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(54) **SYSTEM FOR PERFORMING REMOTE ISCHEMIC CONDITIONING**
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(73) Assignee: **CellAegis Devices Inc.**, Mississauga, Ontario (CA)

(58) **Field of Classification Search**
None
See application file for complete search history.

(56) **References Cited**
U.S. PATENT DOCUMENTS
3,552,383 A 1/1971 Krueger et al.
4,106,002 A 8/1978 Hogue, Jr.
(Continued)

FOREIGN PATENT DOCUMENTS
CN 201098315 8/2008
CN 201098315 Y 8/2008
(Continued)

OTHER PUBLICATIONS
Addison et al., "Noninvasive remote ischemic preconditioning for global protection of skeletal muscle against infarction," *Am. J. Physiol. Heart Circ. Physiol.*, vol. 285, pp. 1435-1443 (2003).
(Continued)

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Related U.S. Patent Documents

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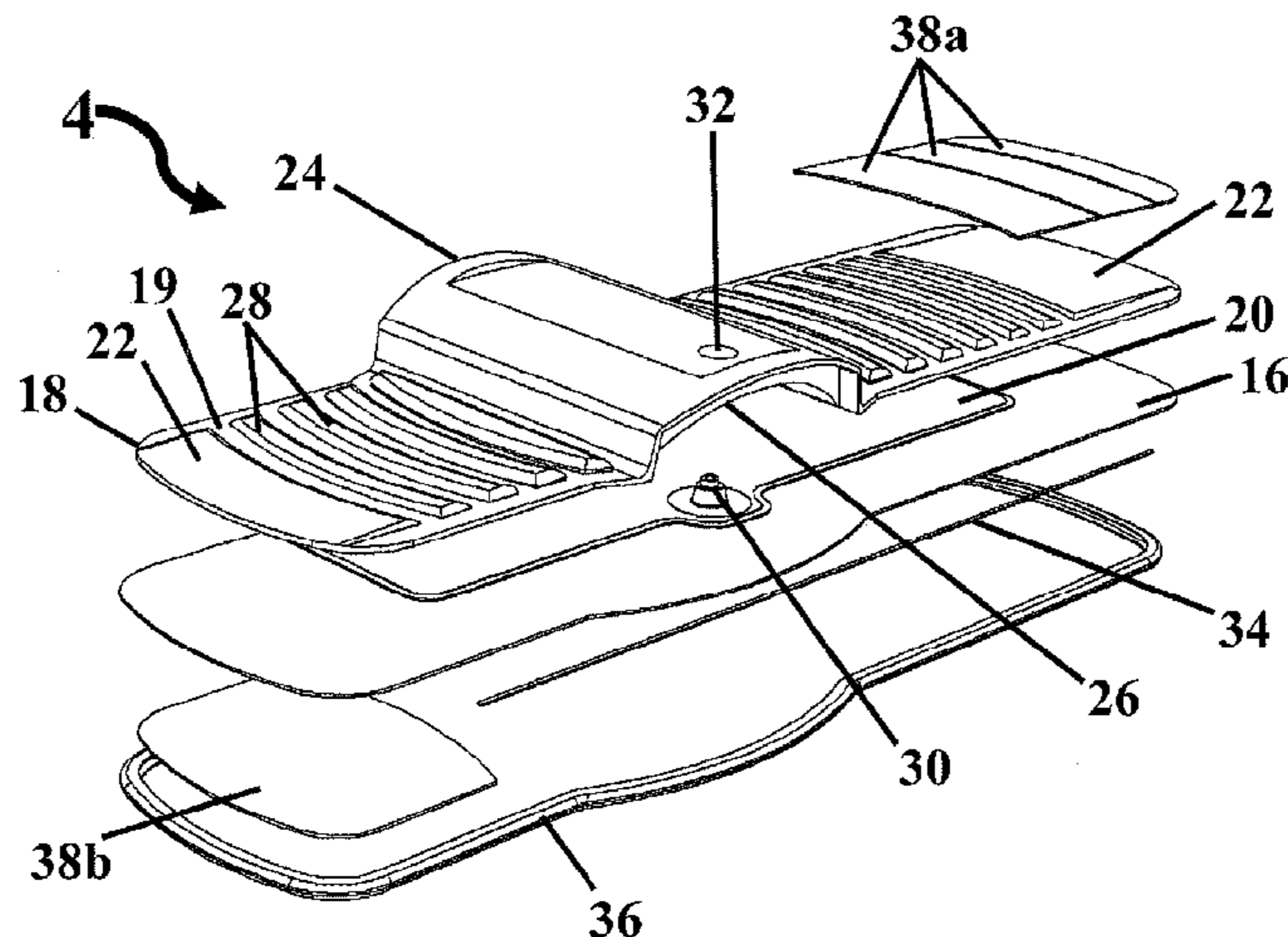
(51) **Int. Cl.**
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CPC **A61H 9/0092** (2013.01); **A61B 5/02233** (2013.01); **A61B 17/1325** (2013.01); **A61B 17/1355** (2013.01); **A61H 9/0078** (2013.01)

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(57) **ABSTRACT**
A system for performing remote ischemic conditioning includes an inflatable cuff configured to encircle a limb of a subject and a controller removably attached to the cuff. The controller includes a pump; a manifold in fluid communication with the pump; a connector in fluid communication with the manifold and in removable fluid communication with the inflatable cuff; a pressure sensor; and a control circuit configured to implement a remote ischemic conditioning treatment protocol.

40 Claims, 7 Drawing Sheets



US RE47,219 E

(51)	Int. Cl.		8,790,266 B2	7/2014	Caldarone et al. .. A61H 9/0078 600/490
	<i>A61B 5/022</i>	(2006.01)	8,911,469 B2	12/2014	Raheman
	<i>A61B 17/132</i>	(2006.01)	8,986,342 B2 *	3/2015	Naghavi A61B 17/1355 606/201
(56)	References Cited		9,119,759 B2 *	9/2015	Caldarone A61H 9/0078
	U.S. PATENT DOCUMENTS		9,119,761 B2 *	9/2015	Caldarone A61H 9/0078
			9,205,019 B2 *	12/2015	Ganske A61B 17/1325
			9,393,025 B2 *	7/2016	Caldarone A61B 17/132
	4,206,764 A	6/1980 Williams	9,439,574 B2 *	9/2016	McCombie A61B 5/02427
	4,294,261 A	10/1981 Baker et al.	9,492,094 B2 *	11/2016	Kitamura A61B 5/022
	4,321,929 A	3/1982 Lemelson et al.	9,610,213 B2 *	4/2017	Leschinsky A61B 5/02208
	4,629,433 A	12/1986 Magid et al.	9,723,985 B2 *	8/2017	Ono A61B 5/0002
	4,664,651 A	5/1987 Weinschenker et al.	9,743,744 B2 *	8/2017	Maier A45F 5/02
	4,690,151 A	9/1987 Utsunomiya et al.	2001/0029389 A1	10/2001	Kim et al.
	4,967,758 A	11/1990 Masciarotte	2003/0013974 A1	1/2003	Natarajan et al.
	5,072,736 A	12/1991 Ogawa et al.	2003/0065270 A1	4/2003	Raines et al.
	5,135,003 A	8/1992 Souma	2003/0176795 A1	9/2003	Harris et al.
	5,201,758 A	4/1993 Glover	2003/0216651 A1	11/2003	Burns et al.
	5,267,565 A	12/1993 Beard et al.	2003/0233118 A1	12/2003	Hui
	5,569,304 A	10/1996 Ulrich	2004/0044290 A1	3/2004	Ward et al.
	5,571,075 A	11/1996 Bullard et al.	2004/0064076 A1	4/2004	Bilgi et al.
	5,634,467 A	6/1997 Nevo	2004/0102818 A1	5/2004	Hakky et al.
	5,643,315 A	7/1997 Daneshvar	2004/0241634 A1	12/2004	Millis et al.
	5,651,369 A	7/1997 Tomita	2004/0255956 A1	12/2004	Vinten-Johansen
	5,687,732 A	11/1997 Inagaki et al.	2005/0004476 A1	1/2005	Payvar et al.
	5,830,198 A *	11/1998 Henniges A61M 1/0023 604/118	2005/0070405 A1	3/2005	Egger
			2005/0159640 A1	7/2005	Barbut et al.
	5,970,548 A	10/1999 Welch	2005/0171444 A1	8/2005	Ono et al.
	6,152,881 A	11/2000 Raines et al.	2005/0177078 A1	8/2005	Loeb et al.
	6,210,423 B1	4/2001 Kim et al.	2006/0052712 A1	3/2006	Poliac et al.
	6,245,023 B1	6/2001 Clemmons	2006/0052713 A1	3/2006	Poliac et al.
	6,251,080 B1 *	6/2001 Henkin et al. A61B 5/02233 600/490	2006/0052714 A1	3/2006	Poliac et al.
			2006/0058717 A1	3/2006	Hui et al.
	6,344,025 B1 *	2/2002 Inagaki et al. A61B 5/0002 600/485	2006/0100639 A1	5/2006	Levin et al.
			2006/0142663 A1	6/2006	Sawanoi et al.
	6,485,429 B2	11/2002 Forstner	2007/0005106 A1	1/2007	Adducci
	6,550,482 B1	4/2003 Burbank et al.	2007/0055188 A1	3/2007	Avni et al.
	6,626,840 B2	9/2003 Drzewiecki et al.	2007/0135836 A1	6/2007	McEwen et al.
	6,702,720 B2	3/2004 Dardik	2007/0150005 A1	6/2007	Sih et al.
	6,719,704 B2	4/2004 Narimatsu et al.	2007/0197943 A1	8/2007	Hakonson et al.
	6,858,012 B2	2/2005 Burns et al.	2007/0247304 A1	10/2007	Bonnefin et al.
	6,905,456 B1	6/2005 Brunner et al. A61H 9/0078 600/16	2008/0077176 A1	3/2008	Hanlon et al. A61H 9/0078 606/201
	6,962,599 B2	11/2005 Hui et al.	2008/0139949 A1	6/2008	Caldarone et al.
	7,004,907 B2	2/2006 Banet et al.	2008/0222769 A1	9/2008	Natonson et al.
	7,018,335 B2	3/2006 Kario et al.	2009/0036785 A1	2/2009	Danielsson
	7,048,702 B2	5/2006 Hui	2009/0124912 A1	5/2009	McEwen et al.
	7,111,346 B2	9/2006 Inman et al.	2009/0137884 A1	5/2009	Naghavi et al.
	7,166,077 B2	1/2007 Millay et al.	2009/0287069 A1	11/2009	Naghavi et al.
	7,228,576 B2	6/2007 Inman et al.	2009/0318818 A1	12/2009	Whitaker et al.
	7,314,478 B2	1/2008 Hui	2009/0324748 A1	12/2009	Dobson
	7,338,410 B2	3/2008 Dardik et al.	2010/0081941 A1	4/2010	Naghavi et al.
	7,374,540 B2	5/2008 Schnall et al.	2010/0081977 A1	4/2010	Vess
	7,390,303 B2	6/2008 Dafni	2010/0105993 A1	4/2010	Naghavi et al.
	7,404,221 B2	7/2008 Sackner	2010/0160799 A1	6/2010	Caldarone et al.
	7,427,268 B2	9/2008 Millay et al.	2010/0185220 A1	7/2010	Naghavi et al.
	7,485,131 B2	2/2009 Hovanes et al.	2010/0186752 A1	7/2010	Rixson
	7,517,312 B2	4/2009 Loeb et al.	2010/0268130 A1	10/2010	Khan
	7,689,286 B2	3/2010 Pastore et al.	2010/0292619 A1	11/2010	Redington et al.
	7,717,855 B2	5/2010 Caldarone et al.	2010/0305607 A1	12/2010	Caldarone et al.
	7,885,710 B2	2/2011 Sih et al.	2010/0322467 A1	12/2010	Reed et al.
	RE42,754 E *	9/2011 Lia A61B 5/02233 600/490	2010/0324429 A1 *	12/2010	Leschinsky A61B 5/02208 600/493
	8,114,026 B2 *	2/2012 Leschinsky A61B 5/02208 600/490	2010/0326442 A1	12/2010	Hamilton et al.
			2010/0328142 A1	12/2010	Zoughi et al.
	8,123,694 B2 *	2/2012 Kinsley A61B 5/02141 600/485	2011/0077566 A1	3/2011	Ganapathy
			2011/0152650 A1	6/2011	Donehoo et al.
	8,246,548 B2	8/2012 Naghavi A61B 17/1355 600/481	2011/0190807 A1	8/2011	Redington et al.
			2011/0238107 A1	9/2011	Raheman
	8,672,854 B2 *	3/2014 McCombie A61B 5/0002 600/485	2011/0240043 A1	10/2011	Redington
			2011/0251635 A1	10/2011	Caldarone
	8,753,283 B2 *	6/2014 Leschinsky A61B 5/02208 600/481	2012/0130419 A1	5/2012	Leschinsky
			2012/0277789 A1	11/2012	Caldarone et al. .. A61H 9/0078 606/202
	8,764,789 B2 *	7/2014 Ganske et al. A61B 17/1325 600/485	2013/0317581 A1	11/2013	Redington
	8,783,499 B2 *	7/2014 Lacy B65F 1/062 220/495.06			

(56)

References Cited

U.S. PATENT DOCUMENTS

2014/0024986 A1 1/2014 Souma
2014/0296756 A1 10/2014 Ganske et al.

FOREIGN PATENT DOCUMENTS

CN	200820123637	11/2008
CN	101317805	12/2008
CN	101317805 A	12/2008
CN	201316381	9/2009
CN	201316381 Y	9/2009
EP	0 960 598	12/1999
EP	0 960 598 A1	12/1999
EP	1 016 379	5/2000
EP	1 249 218	10/2002
EP	1 249 218 A2	10/2002
EP	2 168 553	3/2010
EP	2 301 496	3/2011
GB	1 323 365	7/1973
JP	2001221 A	1/1990
JP	07-051276	2/1995
JP	2001505472	4/2001
JP	2001505472 A	4/2001
JP	2002156773 A	5/2002
JP	2002539879	11/2002
JP	2002539879 A	11/2002
RU	2 253 429	6/2005
RU	2 253 429 C1	6/2005
WO	WO 83/00995	3/1983
WO	WO 83/00995 A1	3/1983
WO	WO 91/18571	12/1990
WO	WO 91/18571	12/1991
WO	WO 98/30144	7/1998
WO	WO 98/30144 A1	7/1998
WO	WO 00/57776	10/2000
WO	WO 00/57776 A1	10/2000
WO	WO 2005/011503	2/2005
WO	WO 2005/011503 A1	2/2005
WO	WO 2005/051250	6/2005
WO	WO 2005/077265	8/2005
WO	WO 2005/077265 A1	8/2005
WO	WO 2006/024871	3/2006
WO	WO 2006/024871 A1	3/2006
WO	WO 2006/030441	3/2006
WO	WP 2006/030441 A2	3/2006
WO	WO 2006/061825	6/2006
WO	WO 2006/061825 A2	6/2006
WO	WO 2007/085816	8/2007
WO	WO 2007/085828	8/2007
WO	WO 2007/087707	8/2007
WO	WO 2008/148045	12/2008
WO	WO 2008/148062	12/2008
WO	WO 2008/148062 A1	12/2008
WO	WP 2008/148045 A1	12/2008
WO	WO 2009/049103	4/2009
WO	WO 2010/132115	11/2010
WO	WO 2010/132115 A1	11/2010
WO	WO 2011/005538	1/2011
WO	WO 2011/005538 A1	1/2011
WO	WO 2012/024342	2/2012

OTHER PUBLICATIONS

Ali et al., Remote ischemic preconditioning reduces myocardial and renal injury after elective abdominal aortic aneurysm repair: a randomized controlled trial, *Circulation*, vol. 116, 11 Suppl., pp. 98-105 (Sep. 2007).

Bartekova et al., "Liver ischemia induced remote preconditioning: role of cardioprotective proteins," ISHR-ES Meeting, *J. Mol. Cell Cardiol.*, vol. 38, Issue No. 6, p. 1004 (Jun. 21-25, 2005).

Botker et al., Remote ischaemic conditioning before hospital admission, as a complement to angioplasty, and effect on myocardial salvage in patients with acute myocardial infarction: a randomised trial, *Lancet*, vol. 375, Issue No. 9716, pp. 727-734 (Feb. 2010).

Brzozowski et al., "Ischemic preconditioning of remote organs attenuates gastric ischemia—reperfusion injury through involvement of prostaglandins and sensory nerves," *Eur. J. Pharmacol.*, vol. 499, Issue Nos. 1-2, pp. 201-213 (Sep. 2004).

Cheung et al., "Randomized controlled trial of the effects of remote ischemic preconditioning on children undergoing cardiac surgery: first clinical application in humans," *J. Am. Coll. Cardiol.*, vol. 47, Issue No. 11, pp. 2277-2282 (Jun. 2006).

Dickson et al., "Rabbit heart can be "preconditioned" via transfer of coronary effluent," *Am. J. Physiol.*, vol. 277, Issue No. 6, Pt. 2, pp. H2451-H2457 (Dec. 1999).

Dong et al., "Limb ischemic preconditioning reduces infarct size following myocardial ischemia-reperfusion in rats," vol. 56, Issue No. 1, pp. 41-46 (Feb. 2004) [Chinese].

Dong et al., "Limb ischemic preconditioning reduces infarct size following myocardial ischemia-reperfusion in rats," vol. 56, Issue No. 1, pp. 41-46 (Feb. 2004) [English abstract].

Gho et al., "Myocardial protection by brief ischemia in noncardiac tissue," *Circulation*, vol. 94, Issue No. 9, pp. 2193-2200 (Nov. 1996).

Hausenloy et al., "Effect of remote ischaemic preconditioning on myocardial injury in patients undergoing coronary artery bypass graft surgery: a randomised controlled trial," *Lancet*, vol. 370, Issue No. 9587, pp. 575-579 (Aug. 2007).

Hausenloy et al., "Preconditioning and postconditioning: underlying mechanisms and clinical application," *Atherosclerosis*, vol. 204, Issue No. 2, pp. 334-341 (Jun. 2009).

Hausenloy et al., "The therapeutic potential of ischemic conditioning: an update," *Nat. Rev. Cardiol.*, vol. 8, Issue No. 11, pp. 619-629 (Jun. 2011).

Hoole et al., "Cardiac Remote Ischemic Preconditioning in Coronary Stenting (Crisp Stent) Study: a prospective, randomized control trial" *Circulation*, vol. 119, Issue No. 6, pp. 820-827 (Feb. 2009).

Jenkins et al., "Ischaemic preconditioning reduces troponin T release in patients undergoing coronary artery bypass surgery," *Heart*, vol. 77, Issue No. 4, pp. 314-318 (Apr. 1997).

Kharbanda et al., "Ischemic preconditioning prevents endothelial injury and systemic neutrophil activation during ischemia-reperfusion in humans in vivo," *Circulation*, vol. 103, Issue No. 12, pp. 1624-1630 (Mar. 2001).

Kharbanda et al., "Remote ischaemic preconditioning protects against cardiopulmonary bypass-induced tissue injury: a preclinical study," *Heart*, vol. 92, Issue No. 10, pp. 1506-1511 (Eur. Pub—Jul. 2006).

Kharbanda et al., "Translation of remote ischaemic preconditioning into clinical practice," *Lancet*, vol. 374, Issue No. 9700, pp. 1557-1565 (Oct. 2009).

Kharbanda et al., "Transient limb ischemia induces remote ischemic preconditioning in vivo," *Circulation*, vol. 106, Issue No. 23, pp. 2881-2883 (Dec. 2002).

Konstantinov et al., "Remote ischemic preconditioning of the recipient reduces myocardial ischemia-reperfusion injury of the denervated donor heart via a Katp channel-dependent mechanism," *Transplantation*, vol. 79, Issue No. 12, pp. 1691-1695 (Jun. 2005).

Konstantinov et al., "The remote ischemic preconditioning stimulus modifies inflammatory gene expression in humans," *Physiol Genomics*, vol. 19, No. 1, pp. 143-150 (Sep. 2004).

Konstantinov et al., "The remote ischemic preconditioning stimulus modifies gene expression in mouse myocardium," *J. Thorac. Cardiovasc. Surg.*, vol. 130, Issue No. 5, pp. 1326-1332 (Nov. 2005).

Lang et al., "Myocardial preconditioning and remote renal preconditioning—identifying a protective factor using proteomic methods?," *Basic Res. Cardiol.*, vol. 101, Issue No. 2, pp. 149-158 (Mar. 2006).

Laskey et al., "Frequency and clinical significance of ischemic preconditioning during percutaneous coronary intervention," *J. Am. Coll. Cardiol.*, vol. 24, Issue No. 6, pp. 998-1003 (Sep. 2003).

Leesar et al., "Nonelectrocardiographic evidence that both ischemic preconditioning and adenosine preconditioning exist in humans," *J. Am. Coll. Cardiol.*, vol. 42, Issue No. 3, pp. 437-435 (Aug. 2003).

(56)

References Cited

OTHER PUBLICATIONS

Leesar et al., "Preconditioning of human myocardium with adenosine during coronary angioplasty," *Circulation*, vol. 95, Issue No. 11, pp. 2500-2507 (Jun. 1997).

Loukogeorgakis et al., "Remote ischemic preconditioning provides early and late protection against endothelial ischemia-reperfusion injury in humans: role of the autonomic nervous system," *J. Am. Coll. Cardiol.*, vol. 46, Issue No. 3, pp. 450-456 (Aug. 2005).

Loukogeorgakis et al., "Transient limb ischemia induces remote preconditioning and remote postconditioning in humans by a K(ATP)-channel dependent mechanism," *Circulation*, vol. 116, Issue No. 12, pp. 1386-1395 (Sep. 2007).

McCully et al., "Adenosine-enhanced ischemic preconditioning: adenosine receptor involvement during ischemia and reperfusion," *Am. J. Physiol. Heart Circ. Physiol.*, vol. 280, Issue No. 2, pp. H591-H602 (Feb. 2001).

Murray et al., "Preconditioning with ischemia: a delay of lethal cell injury in ischemic myocardium," *Circulation*, vol. 74, Issue No. 5, pp. 1124-1136 (Nov. 1986).

Nandagopal et al., "Critical role for nitric oxide signaling in cardiac and neuronal ischemic preconditioning and tolerance," *J. Pharmacol. Exp. Ther.*, vol. 297, Issue No. 2, pp. 474-478 (May 2001).

Peng et al., "The protective effects of ischemic and calcitonin gene-related peptide-induced preconditioning on myocardial injury by endothelin-1 in the isolated perfused rat heart," *Life Sci.*, vol. 59, Issue No. 18, pp. 1507-1514 (1996).

Penttila et al., "Ischemic preconditioning does not improve myocardial preservation during off-pump multivessel coronary operation," *Ann. Thorac. Surg.*, vol. 75, Issue No. 4, pp. 1246-1252 (Apr. 2003).

Peralta et al., "Liver ischemic preconditioning: a new strategy for the prevention of ischemia-reperfusion injury," *Transplant Proc.*, vol. 35, Issue No. 5, pp. 1800-1802 (Aug. 2003).

Przyklenk et al., "Regional ischemic 'preconditioning' protects remote virgin myocardium from subsequent sustained coronary occlusion," *Circulation*, vol. 87, Issue No. 3, pp. 893-899 (Mar. 1993).

Redington et al., "Exploring remote ischaemic preconditioning," *Internal Innovation*, pp. 42-44 www.research.media.eu.

Saxena et al., "Remote ischemic conditioning: evolution of the concept, mechanisms, and clinical application," *J. Card. Surg.*, vol. 25, Issue No. 1, pp. 127-134 (Jan.-Feb. 2010).

Schmidt et al., "Intermittent peripheral tissue ischemia during coronary ischemia reduces myocardial infarction through a KATP-dependent mechanism: first demonstration of remote ischemic preconditioning," *Am. J. Physiol. Heart Circ. Physiol.*, vol. 292, Issue No. 4, pp. H1883-H1890 (Apr. 2007).

Schoemaker et al., "Bradykinin mediates cardiac preconditioning at a distance," *Am. J. Physiol. Heart Circ. Physiol.*, vol. 278, Issue No. 5, pp. H1571-1576 (May 2000).

Takarada et al., "Applications of vascular occlusion diminish disuse atrophy of knee extensor muscles," ed. *Sci. Sports. Exerc.*, vol. 32, Issue No. 12, pp. 2035-2039 (Dec. 2000).

Tanaka et al., "Expression of heat shock protein after ischemic preconditioning in rabbit hearts," *Jpn. Circ J.*, vol. 62, Issue No. 7, pp. 512-516 (Jul. 1998).

Tejwani et al., "Tourniquet cuff pressure: The gulf between science and practice," *J. Trauma*, vol. 61, Issue No. 6, pp. 1415-1418 (Dec. 2006).

Tomai et al., "Ischemic preconditioning in humans: models, mediators, and clinical relevance," *Circulation*, vol. 100, Issue No. 5, pp. 559-563 (Aug. 1999).

Wolfrum et al., "Calcitonin gene related peptide mediates cardioprotection by remote preconditioning," *Regul. Pept.*, vol. 127, Issue Nos. 1-3 (Apr. 2005).

Product ad by Delfi Medical Innovations, Inc., (Delfi tourniquet)(2011).

Takarada et al., "Applications of Vascular Occlusion Diminish Disuse Atrophy of Knee Extensor Muscles," Official Journal of the American College of Sports Medicine, Medicine and Science in Sports and Exercise, pp. 2035-2039 (Apr. 2000).

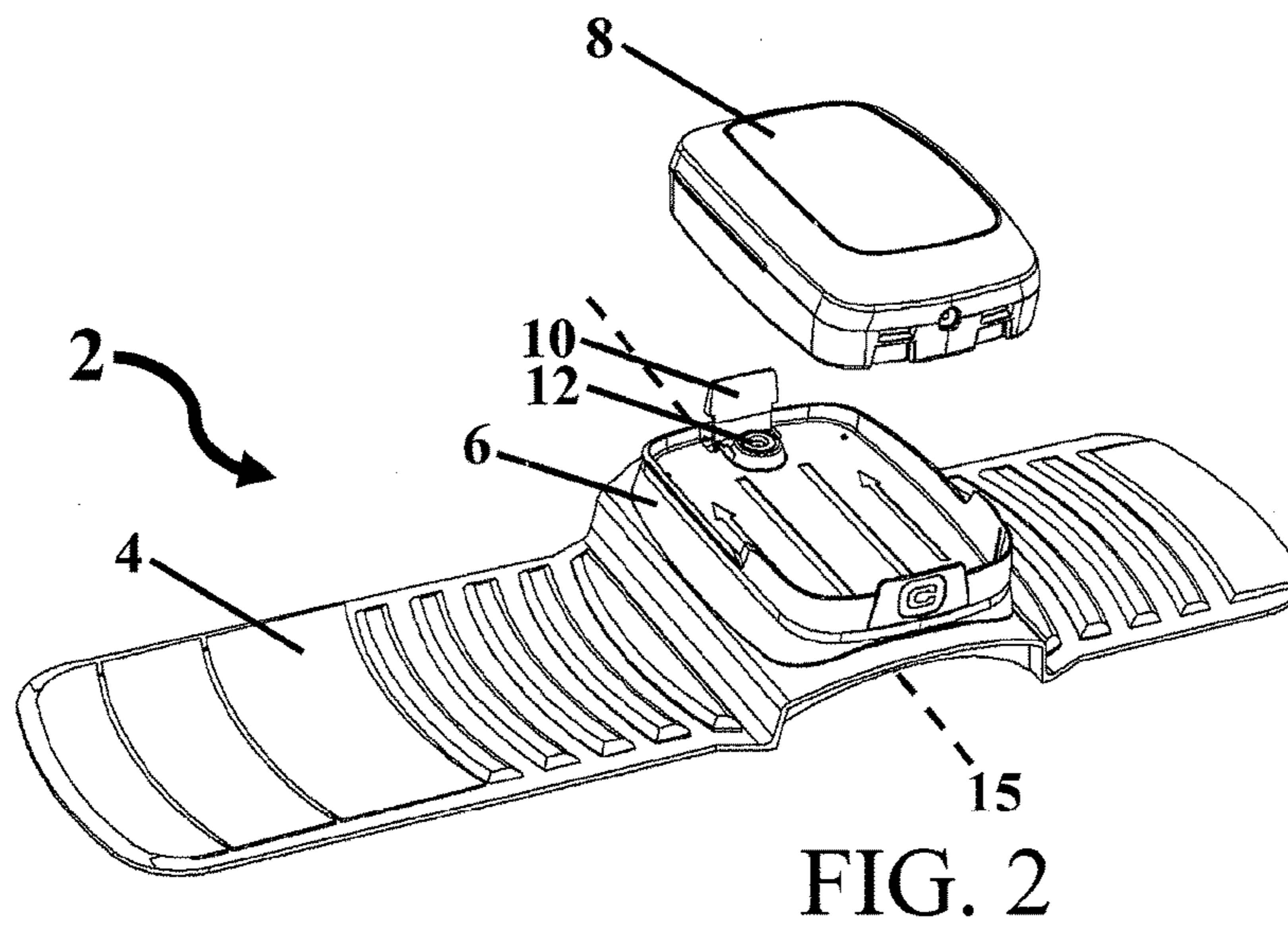
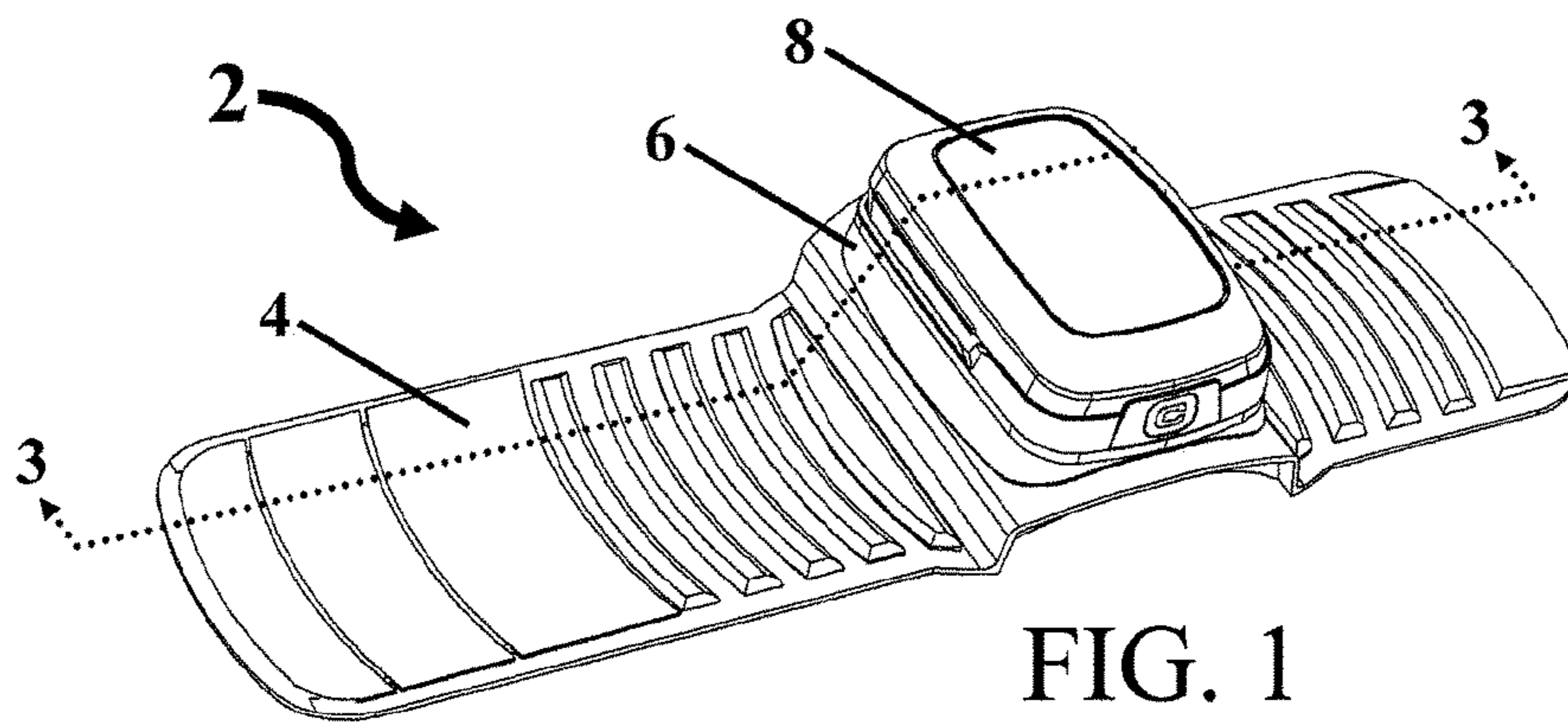
May 29, 2013 Office Action from U.S. Appl. No. 13/542,929.

Search Report from PCT Application No. PCT/US2012/033442, no date.

Written Opinion from PCT Application No. PCT/US2012/033442, no date.

Bötter et al., Upper-limb ischemia during ambulance transfer reduces myocardial perfusion injury in STEMI. *Heartwire*. Mar. 28, 2009. Featured at i2 Session of AAC. Mar. 28-31, 2009. Last Accessed on Mar. 5, 2012 from <http://www.theheart.org/article/951627.do>.

* cited by examiner



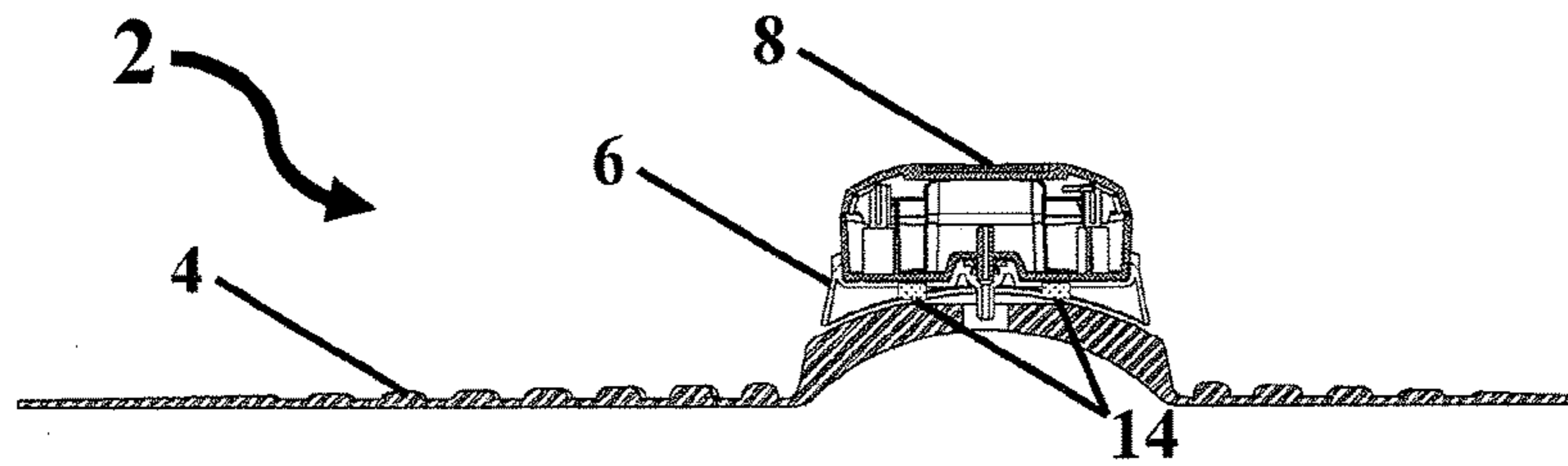


FIG. 3

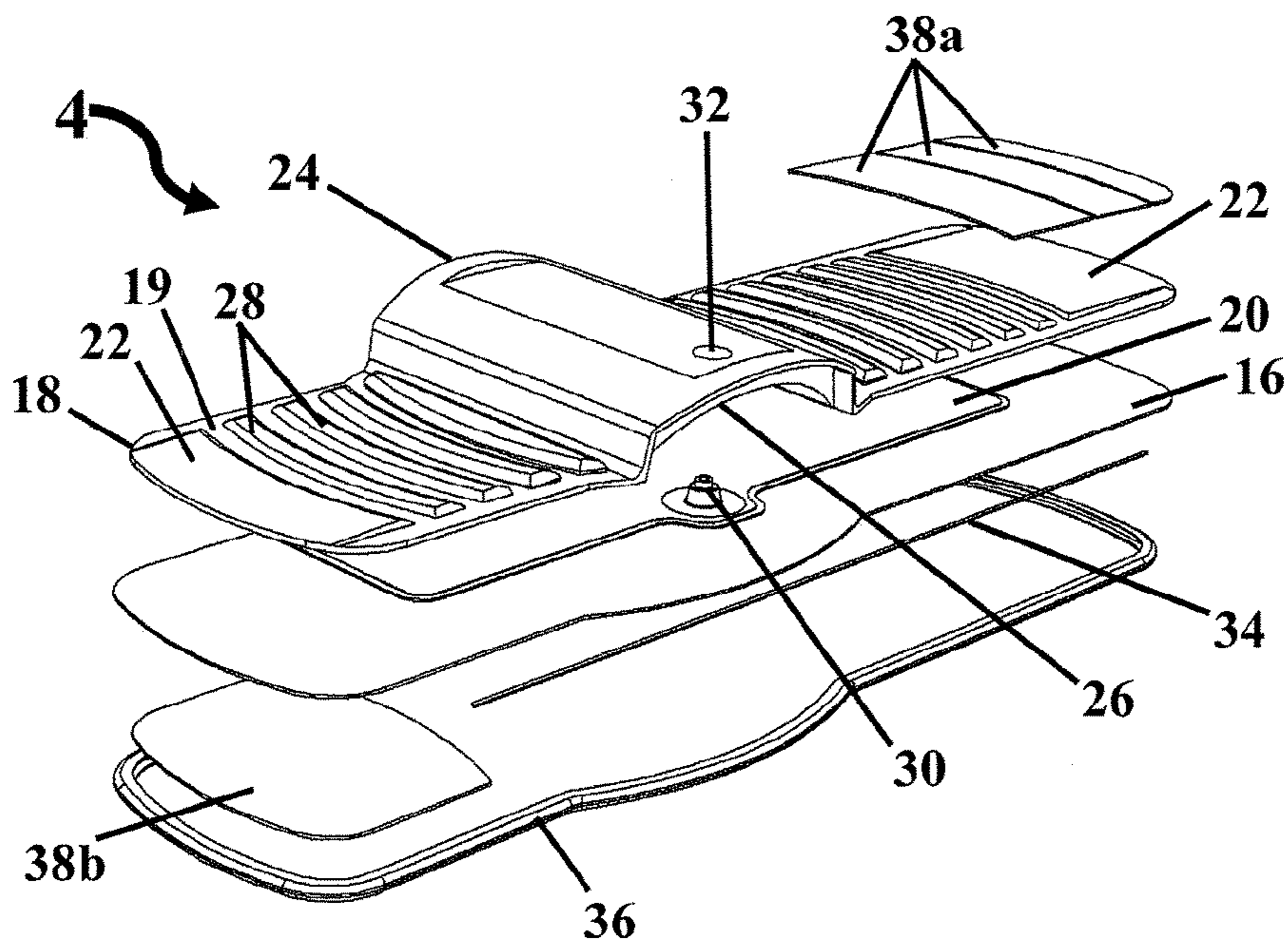
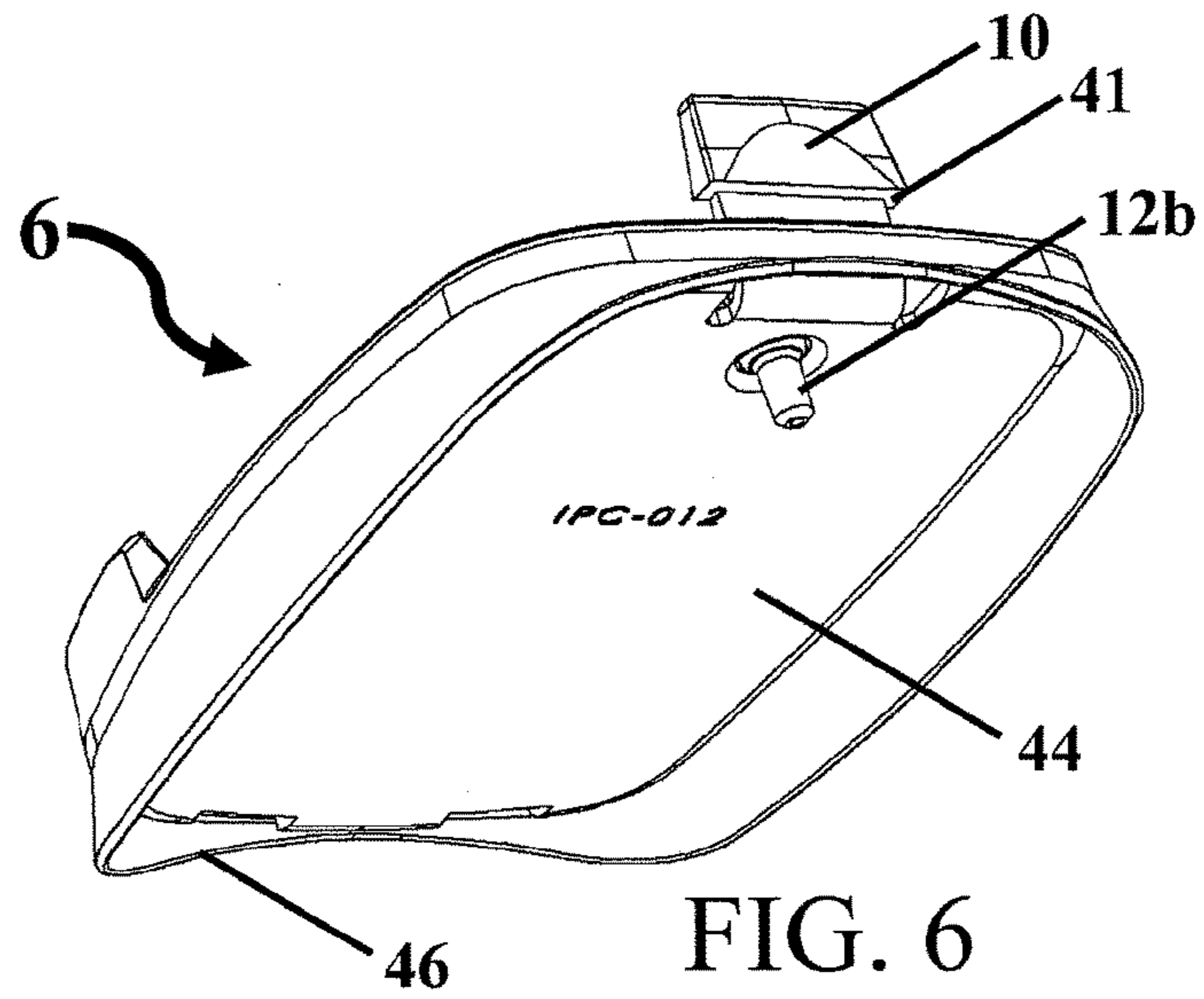
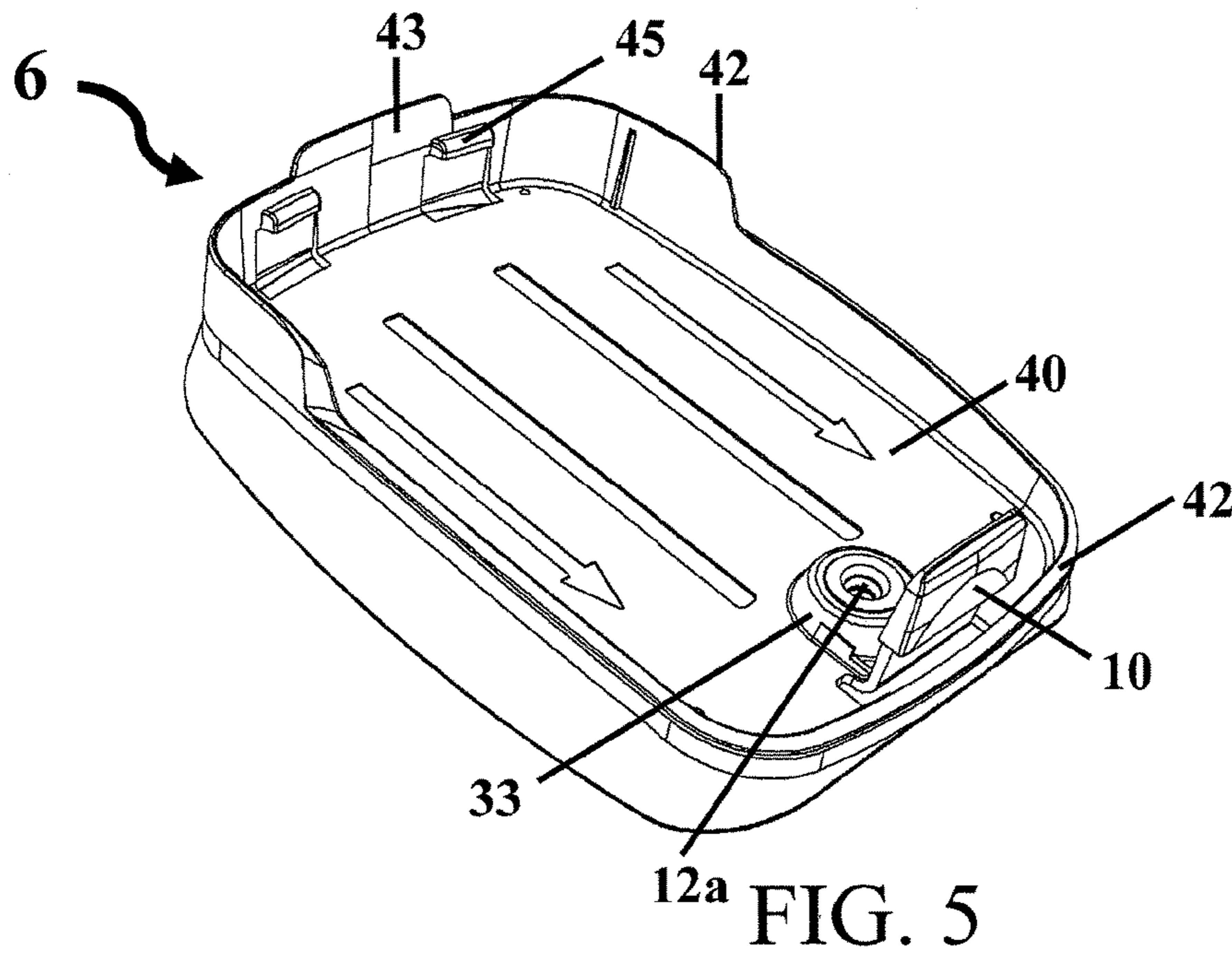


FIG. 4



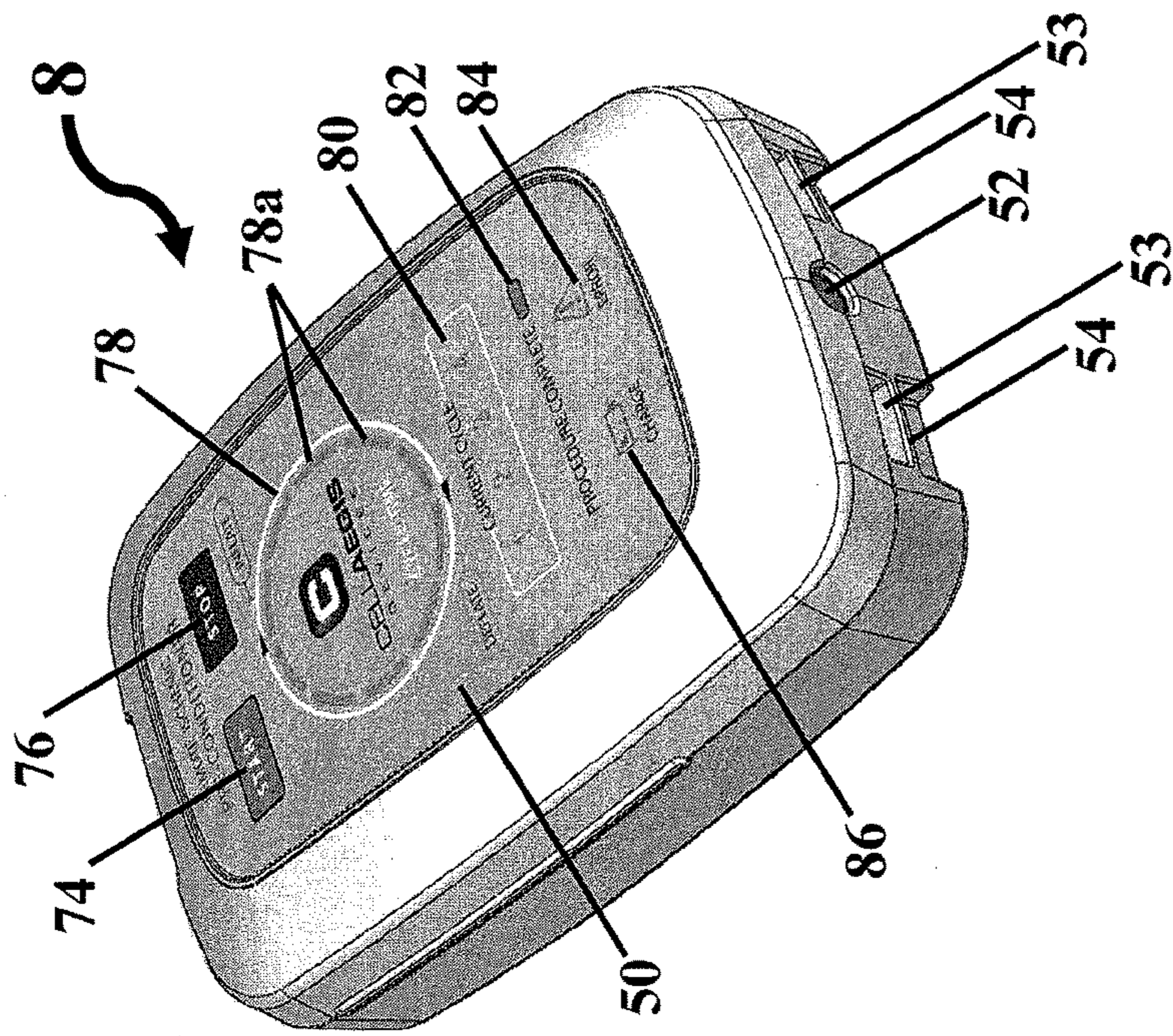


FIG. 7

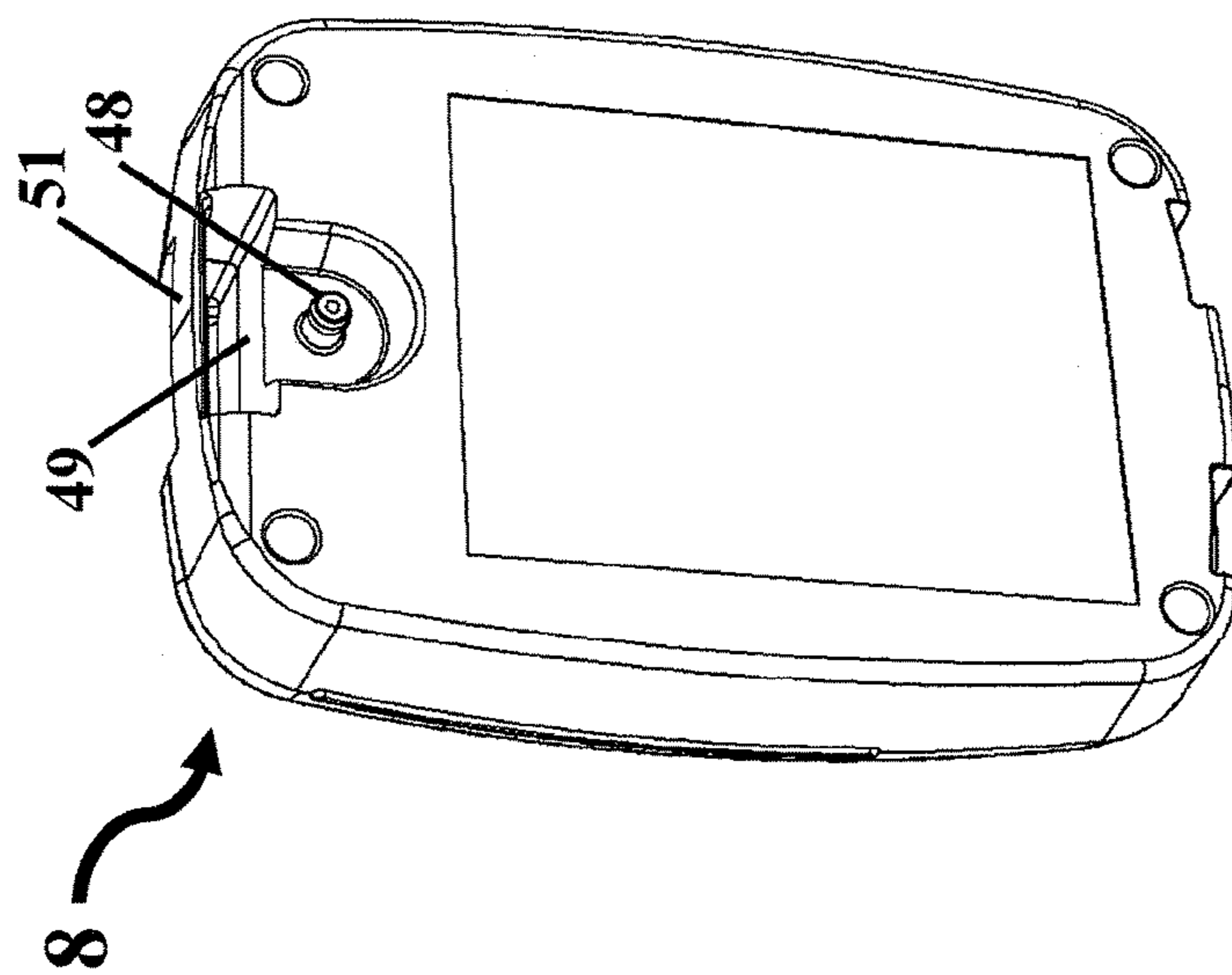
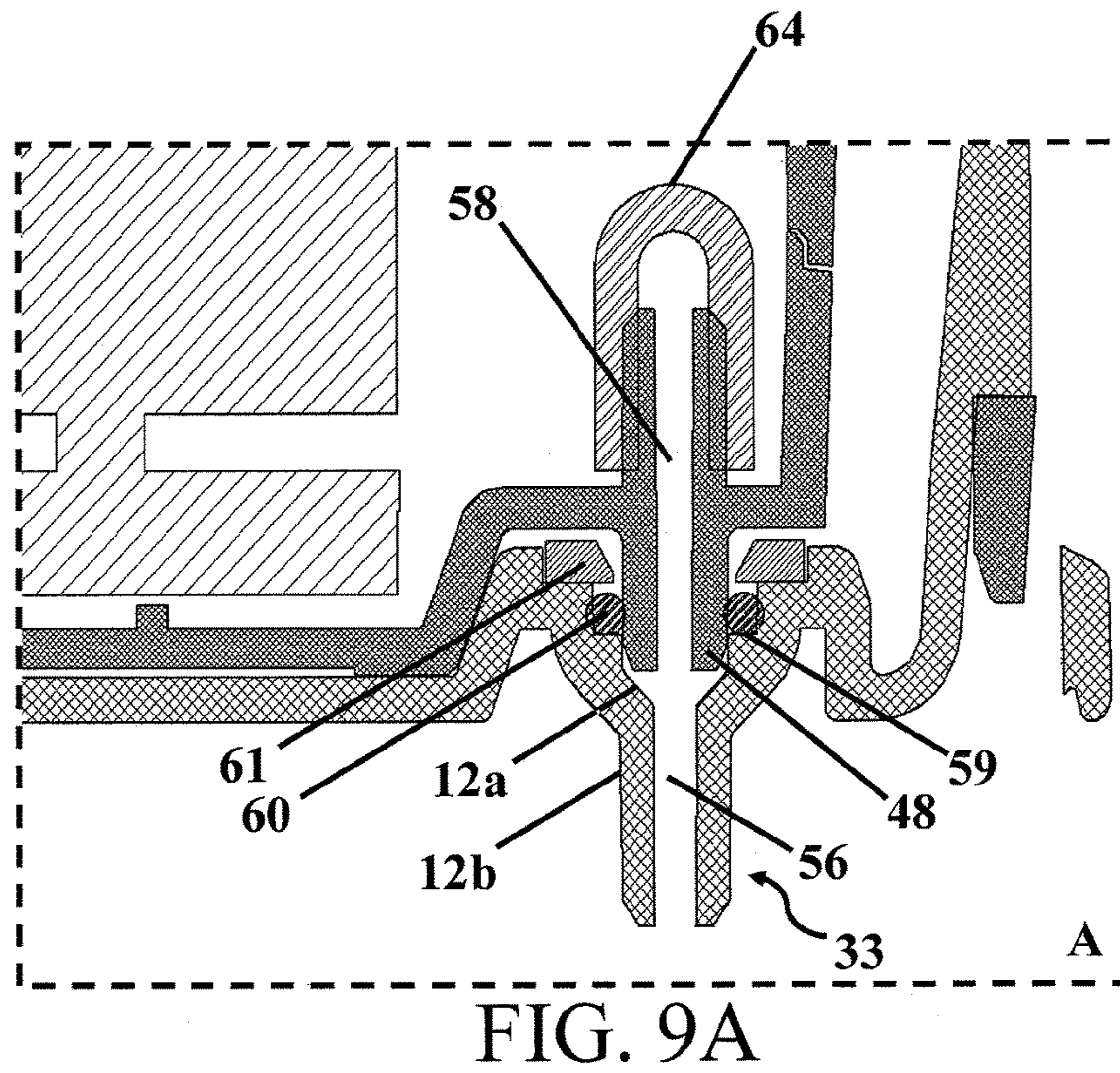
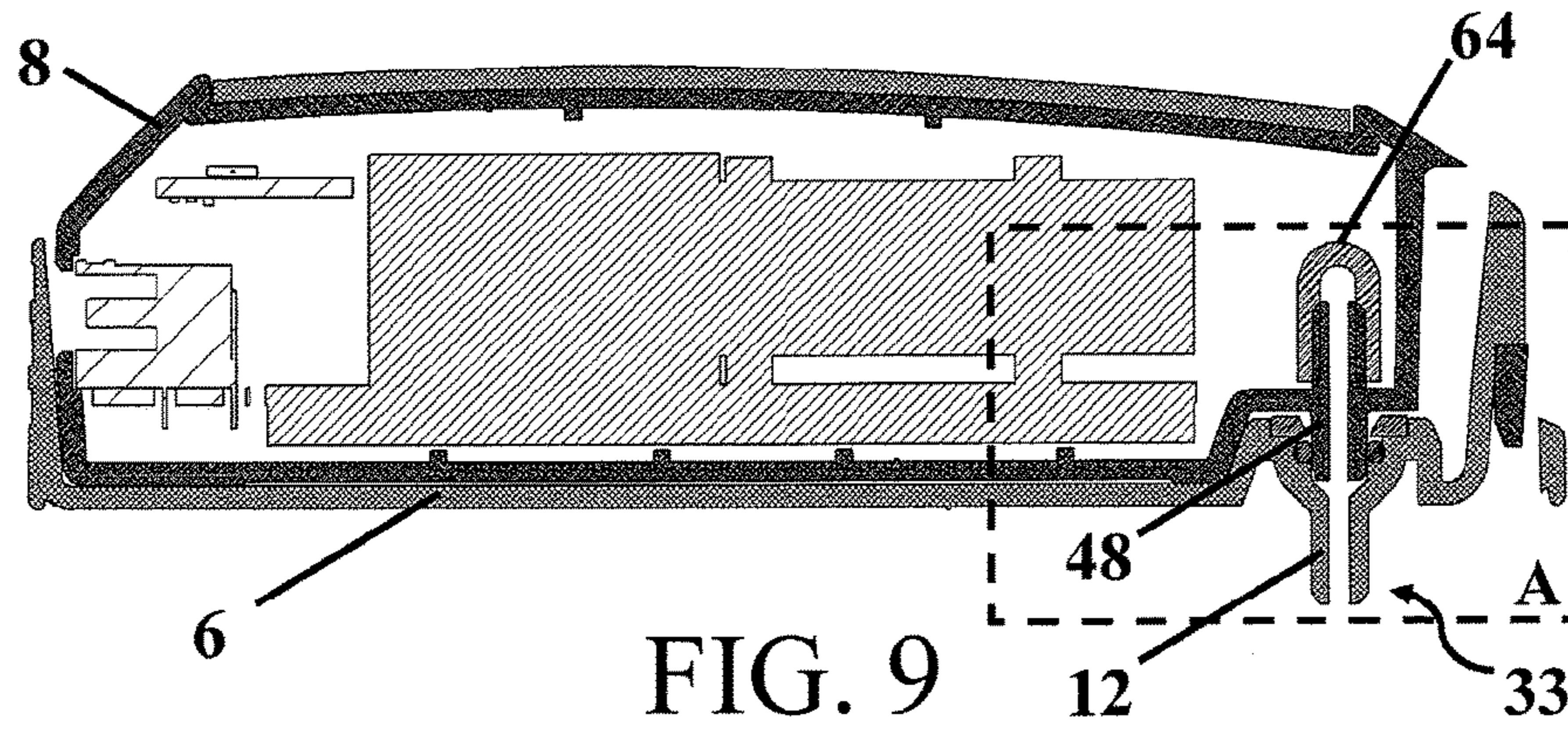


FIG. 8



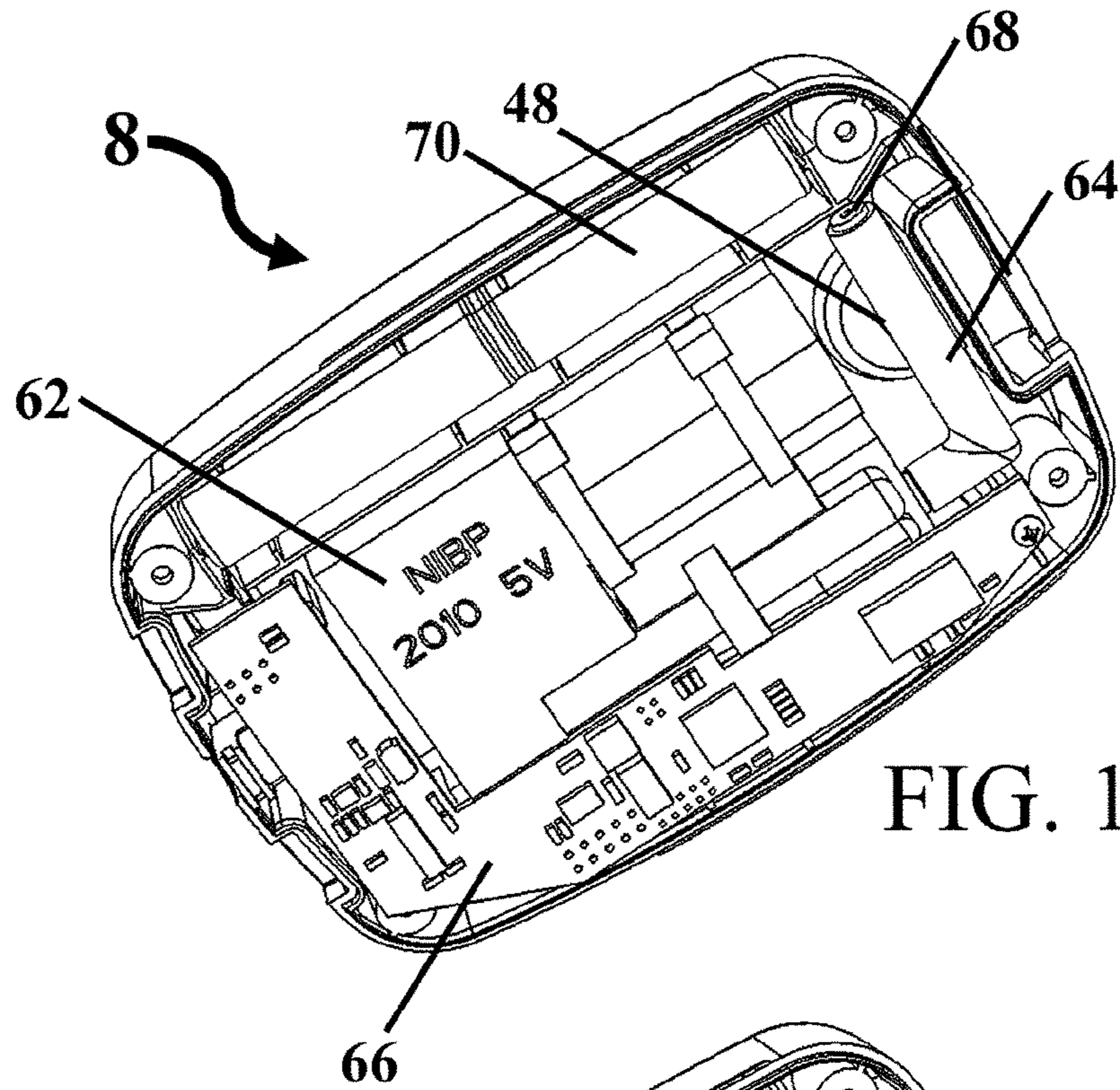
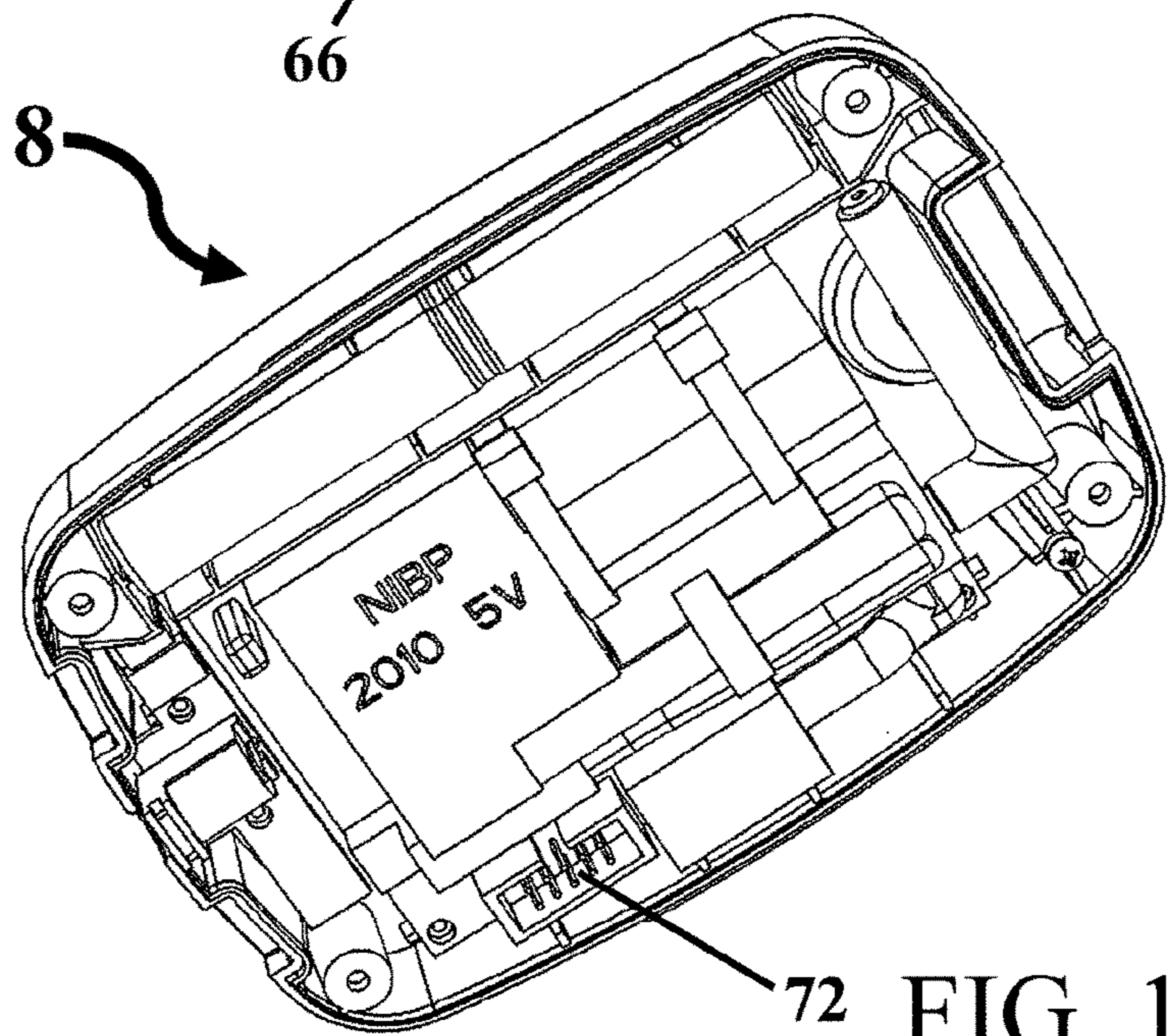


FIG. 10



72 FIG. 11

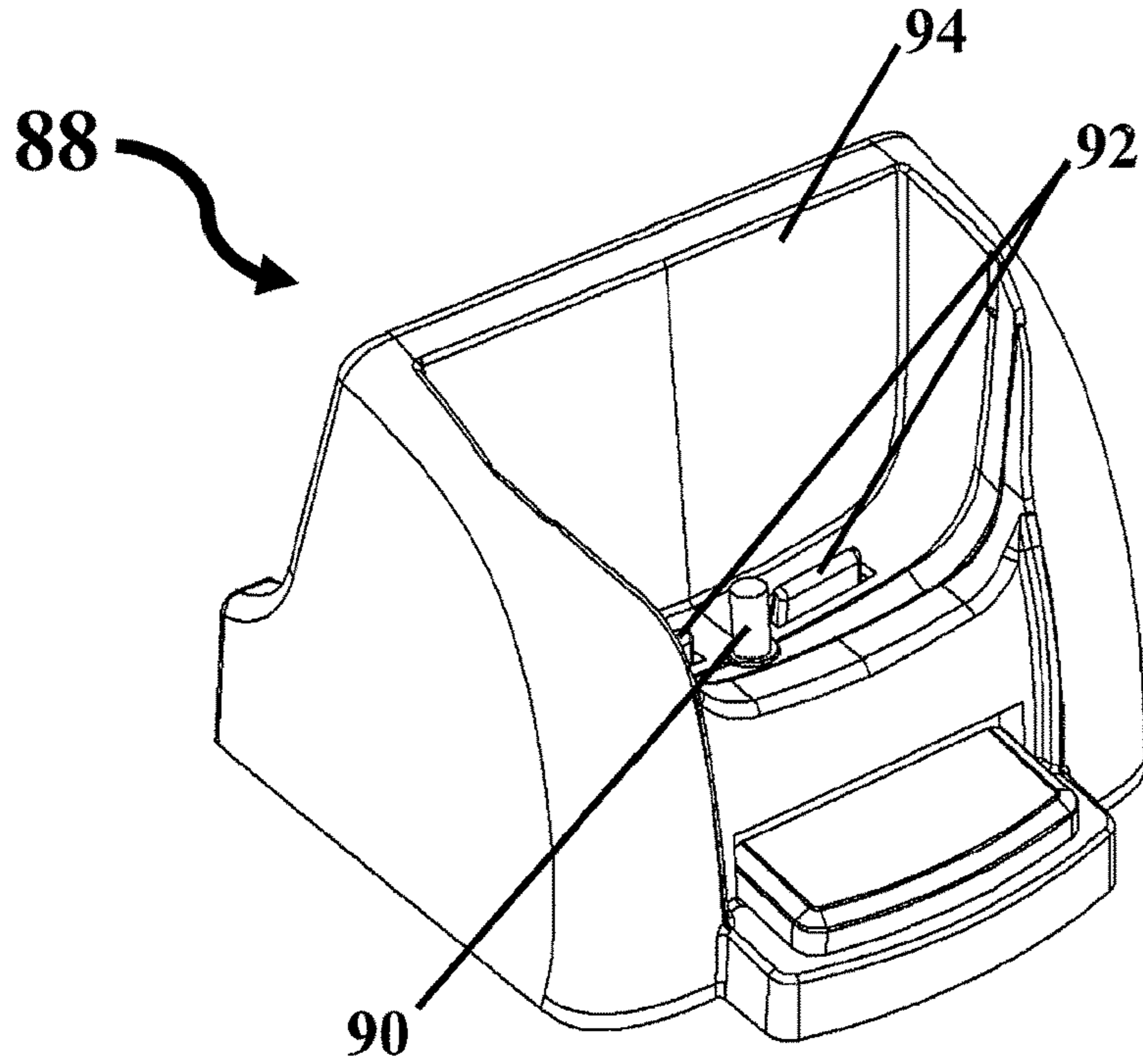


FIG. 12

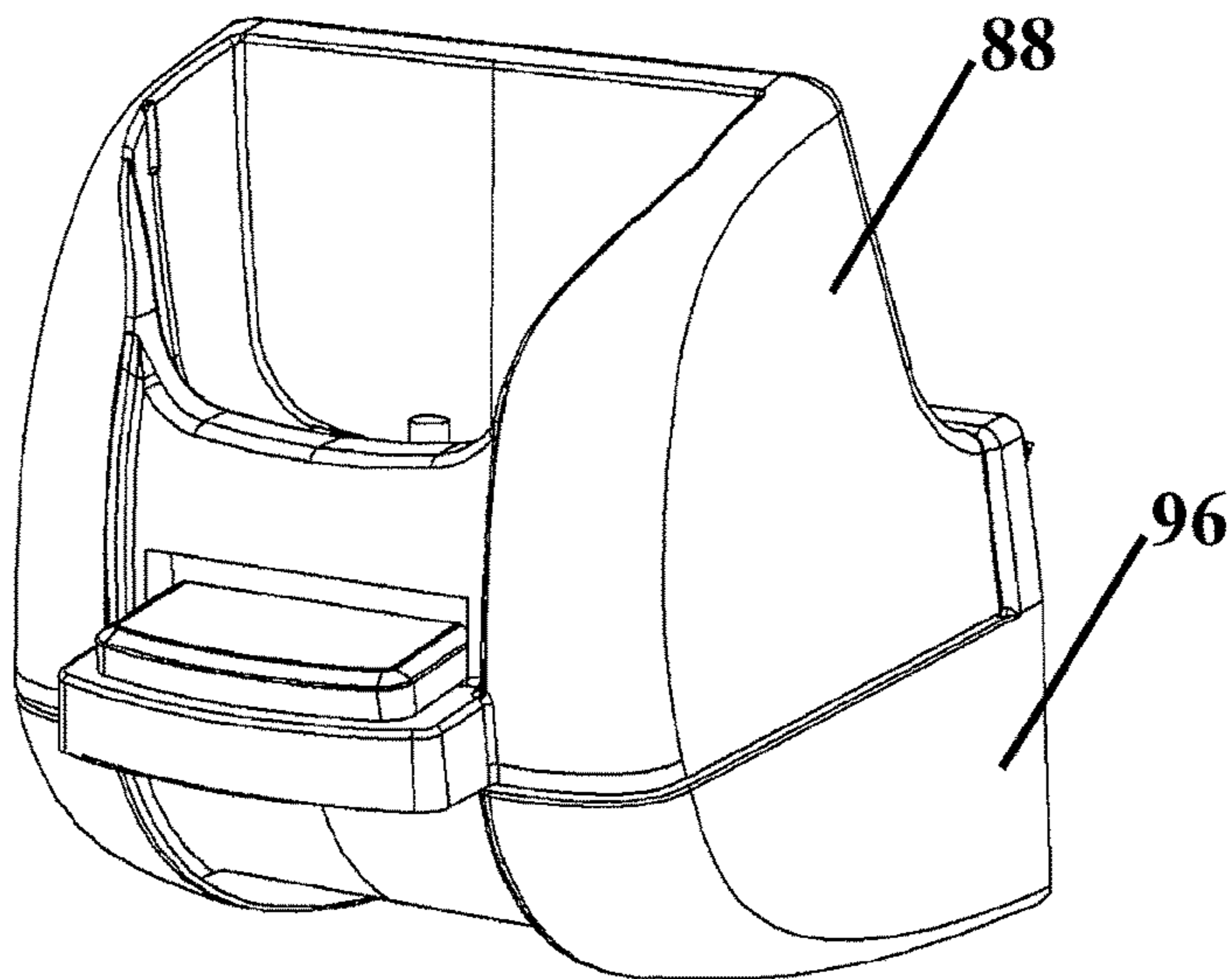


FIG. 13

SYSTEM FOR PERFORMING REMOTE ISCHEMIC CONDITIONING

Matter enclosed in heavy brackets [] appears in the original patent but forms no part of this reissue specification; matter printed in italics indicates the additions made by reissue; a claim printed with strikethrough indicates that the claim was canceled, disclaimed, or held invalid by a prior post-patent action or proceeding.

RELATED APPLICATIONS

This application is a continuation of and claims priority to U.S. patent application Ser. No. 13/088,243, entitled "System For Performing Remote Ischemic Conditioning," filed Apr. 15, 2011, the entire disclosure of which is incorporated herein by reference.

FIELD

This invention relates generally to systems for performing remote ischemic conditioning, and more particularly, to systems for performing remote ischemic conditioning incorporating a removable controller.

BACKGROUND

Ischemic diseases are significant causes of mortality in industrialized nations. It is well established that tissue damage results from ischemia (insufficient blood flow to a tissue) followed by reperfusion (reflow of blood to the tissue). Ischemia and reperfusion cause disturbance of microcirculation with ensuing tissue damage and organ dysfunction. Organs such as the kidney, heart, liver, pancreas, lung, brain and intestine are known to sustain damage following ischemia and reperfusion.

In ischemic conditioning (IC), a tissue or organ or region of a subject's body is deliberately subjected to brief ischemic episodes, followed by brief reperfusion episodes. IC has been found to render the tissue, organ or region resistant to injury during subsequent ischemic episodes. The phenomenon of ischemic conditioning has been demonstrated in most mammalian tissues. IC is now recognized as one of the most potent innate protective mechanisms against ischemia-reperfusion (I-R) injury.

Remote ischemic conditioning (RIC) refers to the deliberate induction of transient ischemia in a subject at a region remote from at least some of the tissue to be protected. Often, RIC includes inducing transient ischemia in a subject's limb to protect organs remote from the limb, such as the myocardium. Myocardial protection has been demonstrated by a variety of remote stimuli, including renal ischemia, liver ischemia, mesenteric artery ischemia, and skeletal muscle hind limb ischemia.

RIC, in the broadest sense, involves deliberate induction of an ischemic period followed by a reperfusion period. The ischemic period may involve complete cessation of blood flow (blood flow occlusion). Such ischemic periods may be induced by applying super-systolic pressures on a region of the body, such as for example a limb. Alternatively, ischemic periods may also be induced by applying a less than systolic pressure.

RIC may be performed prior to (pre-), during (per-) and/or following (post-) an ischemic injury or other injury which

benefits from RIC. RIC has shown benefit in reducing or preventing damage resulting from, myocardial infarction and trauma, inter alia.

SUMMARY

In one aspect, a device for performing RIC includes an inflatable cuff configured to encircle a limb of a subject and a controller removably attached to the cuff. The controller includes a pump; a manifold in fluid communication with the pump; an outlet in fluid communication with the manifold and in removable fluid communication with the inflatable cuff; a pressure sensor; and a control circuit configured to implement a RIC treatment protocol.

In another aspect, a cuff assembly may be adapted to encircle a limb of a subject. The cuff assembly includes an inner layer, an outer layer, and a bladder disposed between the inner layer and the outer layer. The outer layer includes two flexible foam sections spaced apart in a longitudinal direction of the cuff assembly. The outer layer also includes an intermediate section disposed between the two flexible foam sections. The intermediate section may have a greater rigidity than the two flexible foam sections.

In a further aspect, a device includes an inflatable cuff and a controller attachment section. The inflatable cuff may be configured to encircle a limb of a subject. The cuff has an axial direction substantially parallel to an axis of the limb when the cuff is in the fitted state. The controller attachment section may be operatively attached to the cuff by at least one attachment joint oriented substantially parallel to the axial direction of the cuff. The controller attachment section may include a connector adapted for removable attachment of a controller. The controller attachment section may provide fluid communication between the controller and cuff in a location removed from the connector when the controller is in an attached state.

It should be appreciated that all combinations of the foregoing aspects and additional concepts discussed in greater detail below (provided such concepts are not mutually inconsistent) are contemplated as being part of the inventive subject matter disclosed herein.

The foregoing and other aspects, embodiments, and features of the present teachings can be more fully understood from the following description in conjunction with the accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

The accompanying drawings are not intended to be drawn to scale. In the drawings, each identical or nearly identical component that is illustrated in various figures is represented by a like numeral. For purposes of clarity, not every component may be labeled in every drawing. Various embodiments of the invention will now be described, by way of example, with reference to the accompanying drawings, in which:

FIG. 1 is a schematic perspective view of an assembled system for remote ischemic conditioning with a removable controller;

FIG. 2 is a schematic perspective view of the system for remote ischemic conditioning depicted in FIG. 1 with the controller removed;

FIG. 3 is a cross sectional view of the system for remote ischemic conditioning depicted in FIG. 1 taken along the line 3-3 in FIG. 1;

FIG. 4 is an exploded schematic perspective view of the cuff of the system depicted in FIG. 1;

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FIG. 5 is a schematic top perspective view of the controller attachment section of the system depicted in FIG. 1;

FIG. 6 is a schematic bottom perspective view of the controller attachment section of the system depicted in FIG. 1;

FIG. 7 is a schematic bottom perspective view of the controller of the system depicted in FIG. 1;

FIG. 8 is a schematic top perspective view of the controller of the system depicted in FIG. 1;

FIG. 9 is a cross sectional view of the controller and controller attachment section while coupled to the system depicted in FIG. 1;

FIG. 9A is a detailed view of FIG. 9 corresponding to box A of FIG. 9;

FIG. 10 is a schematic perspective view of the controller of the system depicted in FIG. 1 with the cover removed;

FIG. 11 is a schematic perspective view of the controller of the system depicted in FIG. 1 with the cover and PCB removed;

FIG. 12. is a schematic perspective view of a charging cradle to be used with the controller; and

FIG. 13 is a schematic perspective view of the charging cradle of FIG. 12 with an optional wall mount.

DETAILED DESCRIPTION

The illustrative embodiments described herein are not necessarily intended to show all aspects of the invention. Aspects of the invention are not intended to be construed narrowly in view of the illustrative embodiments. It should be appreciated that the various concepts and embodiments introduced above and those discussed in greater detail below may be implemented in any of numerous ways, as the disclosed concepts and embodiments are not limited to any particular manner of implementation. In addition, it should be understood that aspects of the invention may be used alone or in any suitable combination with other aspects of the invention.

In one aspect, a system for performing RIC includes an inflatable cuff, a controller attachment section joined to the cuff, and a controller selectively removable from the controller attachment section. The controller may control the inflation and deflation of the inflatable cuff. Furthermore, the controller may include a control circuit programmed to implement an RIC protocol. In another aspect the cuff may be soft, rigid, and made from thermoformable materials.

Turning now to the figures, several possible embodiments are described in further detail.

FIGS. 1 and 2 illustrate one embodiment of a system 2 for RIC. System 2 may include an inflatable cuff 4, a controller attachment section 6, and a controller 8. In some embodiments, as depicted in FIG. 2, the controller 8 is selectively removable from system 2. The controller attachment section 6 may include an interlocking retaining tab 10 adapted to provide removable attachment of the controller. The controller attachment section may also include a conduit 12 that provides, sealed, fluid communication between the controller 8 and inflatable cuff 6.

In one aspect, cuff 4 is axially rigid while being soft or non-irritating to the skin. In one embodiment, cuff 4 may include an inner layer 16, a layer 18, and a selectively inflatable bladder 20 disposed between layers 16 and 18, as depicted in FIG. 4. Cuff 4 may be adapted to encircle a limb of an individual. Axis 15 represents the approximate center of a circular configuration formed when cuff 4 is wrapped about a patient's limb. An axial direction of cuff 4 corresponds to the approximate direction of axis 15. Cuff 4 has a

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longitudinal direction extending down the length of cuff 4 which is substantially perpendicular to the above defined axial direction. Cuff 4 may also be intended to be a disposable item for use with removable controller 8. Inner layer 16 typically is positioned adjacent to, and often in contact with, the skin of an individual wearing system 2. Since inner layer 16 may be in contact with skin, the inner layer may be made from a soft and/or non-irritating material. The inner layer 16 may be made from a knit, woven, or felted cloth. The cloth may include either natural or synthetic materials. Possible cloths include brushed polyester, brushed nylon, and/or other suitable materials as would be apparent to one of skill in the art. Alternatively, inner layer 16 may be made from a foam. In some embodiments, inner layer 16 may be further adapted to provide moisture absorption, wicking, and/or breathability to cuff 4.

In some embodiments, cuff 4 may include two sections 22 spaced apart in a longitudinal direction and an intermediate section 24 disposed between the sections 22. Intermediate section 24 may be constructed to have a greater rigidity than sections 22. The increased rigidity of the intermediate section 24 may be created either by an inherent material property difference, a difference in the physical construction (e.g. a thicker section and/or inclusion of reinforcing features), or both. In one embodiment, the intermediate section 24 may include a substantially flat outer surface 25 for attachment to the controller attachment section 6. Intermediate section 24 may also include an inner surface 26 which is curved in the longitudinal direction of the cuff 4. The curved inner surface 26 may be constructed so as to generally conform to the curvature of a limb. In some embodiments, the size and curvature of the cuff 4 may be suited for a variety of sizes and ages of patients ranging from neonates to obese adults. The cuff 4 may also be sized for either attachment to an arm or a leg. The intermediate section 24 may be constructed from thermosetting plastics, thermoforming plastics, and/or foamed materials. Sections 22 and the intermediate section 24 may be integrally formed with one another, or they may be formed separately and subsequently joined using any appropriate method including, but not limited to, a sewn seam, ultrasonic welds, adhesives, rivets, clamping structures, and/or mechanically interlocking features. Section 22 may be formed of a foam material or any other suitably flexible yet strong material.

In one embodiment, cuff 4 may also include a plurality of reinforcing structures 28 substantially aligned in the axial direction of the cuff assembly. Reinforcing structures 28 typically may be formed in outer layer 18 of sections 22. Reinforcing structures 28 provide axial rigidity to the cuff 4. The increased axial rigidity provided by reinforcing structures 28 helps to distribute the pressure applied by cuff 4 in the axial direction to provide a substantially uniform pressure across the axial width of the cuff 4. Reinforcing structures 28 may also help to prevent kinks in cuff 4 when it is placed around the arm or leg of an individual. Reinforcing structures 28 may be spaced apart in a longitudinal direction to permit the cuff 4 to easily bend around an encircled limb while still providing increased axial rigidity. Reinforcing structures 28 may be curved or straight in shape in the axial direction. In some embodiments, the reinforcing structures 28 may be integrally formed with the foam in sections 22 such as by the application of heat and/or pressure (e.g. thermoforming) to selectively melt and/or compress portions of the foam in sections 22. The uncompressed and/or unmelted portions of foam in sections 22 form the

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raised reinforcing structures **28**. Alternatively, reinforcing structures **28** may be separately formed and subsequently joined to sections **22**.

Layer **18** may also include a cloth layer **19** applied to an exterior surface. Cloth layer **19** may be formed of a low stretch or non-stretch cloth. The low stretch or non-stretch properties may be an inherent property of the cloth selected. Alternatively, cloth layer **19** may be made from thermoformable materials and may be laminated to the exterior surface of layer **18**. The lamination process may alter the thermoformable fabric to be a low stretch or non-stretch material. In one embodiment, the cloth may be applied to and laminated with layer **18** in a flat layout prior to forming reinforcing structures **28**. Reinforcing structures **28** may subsequently be thermoformed to a final desired shape. The resulting sections **22** may be soft and have low stretch or non-stretch properties. Furthermore, sections **22** may be thermoformable enabling subsequent processing steps.

Selectively inflatable bladder **20** may be disposed between inner layer **16** and layer **18**. Bladder **20** may have a valve **30** arranged and adapted to provide a fluid inlet to the interior of bladder **20**. Valve **30** extends through a hole **32** in the intermediate section **24** of cuff **4**. Valve **30** may be placed in sealed fluid communication with a corresponding structure **33** on controller attachment section **6** which may also be in sealed fluid communication with an outlet **48** of controller **8**. When connected to outlet **48** of controller **8** through structure **33** of the controller attachment section **6**, valve **30** may provide pressurized gas such as air to bladder **20**. In some embodiments, bladder **20** may be a component separate from layers **16** and **18**. Bladder **20** may be formed such as by bonding two separate sheets of thermoplastic polyurethane together. In other embodiments, bladder **20** may be formed from air impermeable layers incorporated into layers **16** and **18** of cuff **4**. Layers of bladder **20** may be bonded together in an air tight manner using any number of methods including adhesives, ultrasonic welding, beads of material around the edges, and/or other appropriate methods as would be apparent to one of skill in the art. Bladder **20** may also be formed as a unitary structure without separate layers.

Layers **16**, **18**, **19**, and bladder **20** of cuff **4** may be held together at their edges in any suitable fashion, such as by a binding material **36** wrapped around the edge of cuff **4** and sewn to cuff **4**, as shown in FIG. **4**. Alternatively, cuff **4** may be held together using adhesives, rivets, ultrasonic welds, or other appropriate methods as would be apparent to one of skill in the art.

In one aspect, it may be desirable to provide a non-slip interface to prevent cuff **4** from moving on the limb of a subject, since system **2** may be worn for protracted periods of time. To provide a non-slip interface, at least one non-slip structure **34** may be disposed on the face of inner layer **16**. The non-slip structure **34** may be printed, glued, sewn, applied as a bead of material using a guided tool, or by hand. The non-slip structure **34** may include, but is not limited to, one or more strips of silicone.

The cuff **4** may also include fasteners to hold the cuff on a limb of a subject and to adjust the circumferential size of the cuff **4** when in the fitted state. Such fasteners include, but are not limited to, hook and loop fasteners, latches, ratchet mechanisms, clasps, snaps, buckles, and other appropriate structures as would be apparent to one of skill in the art. For example, the fastener may be a hook and loop fastener including a plurality of adjacent unconnected hook sections **38a** disposed on layer **18** or **19** and loop sections **38b** disposed on inner layer **16**. Hook sections **38a** may extend in the axial direction of the cuff **4**. The width of each hook

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section **38a**, with respect to the longitudinal direction of the cuff, may be selected to provide a flexible cuff able to wrap around different sized limbs.

The controller attachment section **6** of FIG. **1** is shown in more detail in FIGS. **3**, **5** and **6**. In one embodiment, controller attachment section **6** may include an upper surface **40** for supporting controller **8** in the attached state, a lower surface **44**, and an upstanding wall **42** surrounding surface **40**. A raised portion **43** of upstanding wall **42** may be located adjacent to and block a power inlet **52** of controller **8** in the attached state. By blocking access to power inlet **52** in the attached state, raised portion **43** may prevent use of the device while controller **8** is connected to an external power source. The controller attachment section **6** may also include a connector, such as retaining tab **10**, arranged to provide removable attachment of controller **8**. In one embodiment, tab **10** is mounted at one end to surface **40** and includes a projecting edge **41** spaced from surface **40** that faces outwardly towards wall **42**. Bosses **45** are disposed on wall **42** on the opposite side of section **6** from tab **10**. When controller **8** is attached to attachment section **6**, the upper portion of tab **10** is pushed inwardly away from wall **42** so that it passes through slot **49** that is disposed between the body of controller **8** and an outer band **51**, as shown in FIG. **7**. At the same time, bosses **45** extend into recesses **53** of controller **8**, as shown in FIG. **8**. Tab **10** has sufficient resilience that when snapped into place, this resilience creates an outward bias on tab **10** that causes edge **41** to overlie the upper edge of band **51**. To release controller **8**, the upper portion of tab **10** is again pushed inwardly against its bias toward controller **8** until edge **41** overlies slot **49** and is clear of band **51** at which time controller **8** may be pulled out of attachment section **6** at the end closest to tab **10**.

In one embodiment, lower surface **44** and/or bottom edge **46** of controller attachment section **6** may be disposed on and substantially conform to the shape of an outer surface of cuff **4**. In some embodiments, bottom surface **44** and/or bottom edge **46** of the controller attachment section **6** may be disposed on and substantially conform to the shape of outer surface **25** of intermediate section **24** of cuff **4** shown in FIG. **4**. As shown in FIG. **3**, the controller attachment section **6** may be joined to outer surface **25** of intermediate section **24** of inflatable cuff **4** along lower surface **44** by at least one and typically two attachment joints **14**. In one embodiment, the attachment joint(s) **14** may be oriented substantially parallel to axis **15** of the cuff. The attachment joint **14** may be formed using any appropriate method including, but not limited to, a sewn seam, an ultrasonic weld, an adhesive, and/or rivets. When two or more attachment joints **14** are included, the joints **14** may be spaced apart in the longitudinal direction to allow the cuff **4** to bend and conform to the shape of different sized limbs.

As shown in FIGS. **9** and **9A**, controller attachment section **6** may provide fluid communication between the controller **8** and bladder **20** of cuff **4** via structure **33**. Structure **33** may include a conduit **12** which is provided in a location spaced from retaining tab **10**, when the controller **8** is in an attached state. Conduit **12** fluidly couples controller **8** to valve **30** of bladder **20**. Conduit **12** may include a female section **12a** that is constructed and arranged to mate with an outlet **48** of controller **8** and a male section **12b** that is constructed and arranged to mate with valve **30** of bladder **20**. Outlet **48** may include a fluid conduit **58**. While a male and female connection have been described, the male and female portions could be reversed or even replaced with other comparable fluid connections, such as a tube or the like. A seal, such as O-ring **60**, may be disposed on a

shoulder **59** located in structure **33**. The O-ring **60** may create a gland seal between female section **12a** and outlet **48**. Alternatively, a compression seal with O-ring **60** may be used. A retaining structure **61** may be included in structure **33** to retain O-ring **60**. Retaining structure **61** may be joined to structure **33** using any appropriate method including, but not limited to, press fitting, ultrasonic welding, and/or adhesives.

As shown in FIG. **8**, controller **8** has a front cover **50**, which may include controls and displays, and a power inlet **52**. Guide structures **54** may be included in controller **8** for alignment and/or engagement with a charging mechanism

The internal components of controller **8** are best shown in FIGS. **10** and **11**, where front cover **50** of controller **8** has been removed. Controller **8** may include a pump **62** in fluid communication with a manifold **64**. Manifold **64** is in fluid communication with relief valve **68** and outlet **48**. Controller **8** may also include a printed circuit board (PCB) **66** which may include a control circuit and memory. The controller **8** may also include a pressure sensor associated with the pressurized components of the system and the control circuit. The pressure sensor (not shown) may be incorporated into pump **62** and/or placed in pressure sensing communication with manifold **64**. Furthermore, the pressure sensor may communicate with the control circuit of PCB **66**. The control circuit may be programmed to implement an RIC treatment protocol. The controller may also determine blood pressure during, or as part of, an RIC treatment protocol. To provide convenient mobile usage of system **2**, batteries **70** may be arranged, typically in series, to provide a higher operating voltage. Alternatively, batteries **70** may be in electrical communication with a transformer adapted to provide a higher operating voltage. In one embodiment, the operating voltage may be approximately 5 to 6 VDC. In other embodiments, the operating voltage may be approximately 12 VDC or any other appropriate voltage. As shown in FIG. **11**, PCB **66** may be connected to the other controller components through plug connector **72**.

The control circuit of PCB **66** may be programmed with certain error conditions which may cause the procedure to be aborted or which may cause an indication of the error to appear on a display or which can be used in other known ways. These error conditions may include, but are not limited to: the cuff is not pressurized within a predefined period, such as 20 seconds, 30 seconds, 40 seconds, 50 seconds, or one minute; there is no communication between pump **62** and PCB **66** upon start up; there is no communication between pump **62** and PCB **66** for more than a predefined period, such as two, three, four, or five seconds; multiple consecutive repumps are needed to maintain cuff pressure; pump **62** continues to run and does not respond to an abort signal after a predefined number of retries, such as three, four, or five retries; pressure in cuff **4** is not near zero gage pressure within a predefined period, such as 20 seconds, 30 seconds, 40 seconds, 50 seconds, or one minute after the end of an inflation cycle; pressure in cuff **4** is above a predetermined pressure such as 200, 220, 240 or 260 mmHg for longer than a predefined period, such as 5, 10, 20, or 30 seconds; and the pump **62** CPU does not wake up after a command is sent to it by the control circuit. The error condition may be cleared and/or the system may be reset such as by pressing a stop button **76** on the face of controller **8**.

During usage, controller **8** may be attached to controller attachment section **6** to place controller outlet **48** into fluid communication with cuff **4**. Pressurized gas may then be pumped through controller outlet **48** to inflate the cuff **4**. The

cuff pressure may be controlled by selectively opening valve **68** in response to a command from the control circuitry of PCB **66**. In some embodiments, valve **68** may include a pressure safety relief feature that opens valve **68** in response to an over pressure event during an RIC treatment. In one embodiment, valve **68** opens when the pressure in cuff **4** exceeds 260 mmHg. Valve **68** may open in response to either an error command from the control circuitry of PCB **66**, or the valve **68** may include an automatically actuated mechanical system. Controller **8** may also include a slow continuous relief valve. Such a valve would continuously release gas from inflated bladder **20** at a selected rate lower than the rated flow rate of the pump **62**. The slow continuous release of gas from bladder **20** could be used to deflate bladder **20** in case of a mechanism failure.

In some embodiments, the control circuit of PCB **66** may be programmable by a health professional and/or an end user according to a prescribed treatment protocol. Alternatively, the control circuit may only be programmed at the factory and may not be altered afterwards by the end user. The control circuitry may also include non-volatile memory for the logging and storage of treatment history. A health care professional may be able to access this memory to determine the treatment history of a patient and determine compliance with a prescribed treatment regime. In another embodiment, the controller may send this information via wireless, or hard wired, communication to a separate receiver for patient records, monitoring, or call center purposes. In one embodiment, controller **8** may include a start button **74** and stop button **76**. In some embodiments, the start and stop buttons **74** and **76** may be incorporated into a single button. Controller **8** may also include a hard wired and/or emergency stop button and/or a quick release valve (not shown). In other embodiments, other controls may be included to allow expanded control of an RIC treatment.

In addition to controls, controller **8** may include displays related to the current cycle, the number of cycles left in a treatment, whether the treatment is completed, error signals, charge of the system, and other relevant information. In one embodiment, controller **8** may include a cycle time display **78**. Cycle time display **78** may indicate the remaining portion of the inflation/deflation cycle by using illuminated indicators **78a** arranged in a circular pattern corresponding to a full inflation/deflation cycle. Each indicator **78a** of cycle time display **78** may correspond to a set fraction of the inflation/deflation cycle. When all of the indicators **78a** of cycle time display **78** are illuminated, the inflation/deflation cycle is complete. Alternatively, the indicators **78a** of cycle time display **78** may start a cycle fully illuminated and sequentially turn off as the cycle proceeds. When each indicator **78a** of cycle time display **78** is dark, the particular inflation/deflation cycle is complete. While a circular display has been disclosed, cycle time display **78** could also be arranged in other linear, or non-linear, shapes corresponding to a full cycle. Controller **8** may also include a current cycle display **80**, or a digital numeric display, indicating whether the current cycle is the first, second, third, or other cycle. A procedure complete indicator **82** may be illuminated with a solid color or it may blink when the RIC treatment is complete to indicate the end of the procedure. An error display **84** may indicate when an error has occurred by blinking or being fully illuminated. Alternatively, error display **84** may blink in a preset pattern or display a particular color to indicate which error has occurred. A battery charge indicator **86** may indicate the approximate

charge remaining in the batteries 70, and may also signal that that the remaining charge is only sufficient for one cycle by blinking.

The above described system may be used for implementing an RIC treatment. The treatment includes placing cuff 4 on a limb of a user and attaching controller 8 to controller attachment section 6 on cuff 4. A user may then press start button 74 to initiate the treatment. Once started the control circuitry of PCB 66 monitors the pressure sensor and turns pump 62 on to inflate the cuff 4. The pressure is then increased to a desired pressure, such as a blood flow occlusion pressure. In one embodiment, the control circuitry of PCB 66 maintains the cuff pressure between preselected pressure limits such as 200 mmHg to 210 mmHg. In other embodiments, the control circuitry of PCB 66 may first determine a systolic blood pressure. After determining a systolic blood pressure, the control circuitry of PCB 66 may subsequently initiate the RIC treatment protocol with a desired pressure such as a pressure greater than the measured systolic blood pressure. Regardless of the specific pressure used, the pressure may be maintained for a selected ischemic duration. Ischemic durations may last on the order of seconds or minutes. After completing the ischemic duration, the controller may activate valve 68 to deflate cuff 4 and initiate the reperfusion duration. Reperfusion durations generally last for at least a minute, although shorter reperfusion durations may be used. After completion of the reperfusion duration another RIC cycle may be conducted. An RIC treatment may include a single cycle or multiple cycles. In one embodiment, an RIC treatment may include four cycles with ischemic durations of approximately 5 minutes, and reperfusion durations of approximately 5 minutes. At the end of the last cycle the cuff 4 may deflate within 30 seconds and the controller 8 may confirm a near zero gage pressure prior to shutting down.

In some embodiments, controller 8 may be charged using a charging cradle 88, as shown in FIG. 12. Charging cradle 88 may include a power connector 90 and mating guide structures 92. In one embodiment, mating guide structures 92 on the charging cradle mate with guide structures 54 on the controller. Mating guide structures 92 act as alignment features. In other embodiments, mating guide structures 92 may be actuated when controller 8 is inserted into the charging cradle 88 to turn the power on and off to power connector 90. Charging cradle 88 may also include a raised area 94 to prevent insertion of the controller while controller 8 is connected to cuff 4 or a patient. In addition to the above, charging cradle 88 may optionally connect with a wall mount portion 96 as shown in FIG. 13.

While the present teachings have been described in conjunction with various embodiments and examples, it is not intended that the present teachings be limited to such embodiments or examples. On the contrary, the present teachings encompass various alternatives, modifications, and equivalents, as will be appreciated by those of skill in the art. Accordingly, the foregoing description and drawings are by way of example only.

What is claimed is:

1. A device for remote ischemic conditioning comprising:
 - an inflatable cuff configured to encircle a limb of a subject;
 - a controller removably attached to the cuff, wherein the controller comprises:
 - a manifold configured to provide fluid communication between the controller and the cuff;

- an outlet in fluid communication with the manifold and in removable fluid communication with the inflatable cuff; and
 - a control circuit configured to implement a remote ischemic conditioning treatment protocol; and
- a controller attachment section joined to the cuff, the controller attachment section having a bottom surface that substantially conforms to an outer surface of the cuff, wherein the controller is removably attached to the cuff by selective attachment to the controller attachment section disposed on the cuff, the controller attachment section further comprising:
 - an upper surface for supporting the controller in an attached state;
 - an upstanding wall surrounding the upper surface;
 - a tab mounted at one end of the upper surface and including a projecting edge spaced from the upper surface, the projecting edge facing outwardly toward the upstanding wall; and
 - bosses disposed on the upstanding wall on the opposite side of the controller attachment section from the tab;
 wherein the controller further comprises a slot that is disposed between a body of the controller and an outer band, and wherein the device is arranged such that when the controller is attached to the controller attachment section, an upper portion of the tab is pushed inwardly away from the upstanding wall so that the tab passes through the slot, and the bosses extend into corresponding recesses provided in the controller body.
 2. The device of claim 1, wherein the controller attachment section further includes a conduit that provides sealed, fluid communication between the controller and inflatable cuff.
 3. The device of claim 1, wherein cuff pressure is controllable by selectively opening a valve of the controller in response to a command from control circuitry of the control circuit.
 4. The device of claim 3, wherein the controller attachment section provides fluid communication between the controller and a bladder of the cuff via a structure that includes a conduit that has a female section constructed and arranged to mate with the controller outlet and a male section that is constructed and arranged to mate with a valve of the bladder of the cuff.
 5. The device of claim 1, wherein:
 - an axial direction of the cuff is substantially parallel to an axis of the limb when the cuff is in a fitted state;
 - the controller attachment section is operatively attached to the cuff by at least one attachment joint oriented substantially parallel to the axial direction of the cuff; and
 - the controller attachment section provides fluid communication between the controller and the cuff.
 6. The device of claim 1, wherein the controller comprises a slow continuous relief valve that continually releases gas from the cuff at a flow rate lower than a flow rate of the gas being introduced into the cuff.
 7. The device of claim 1, wherein the controller further comprises at least one valve configured to open in response to an overpressure event, or in response to an error command from the control circuit.
 8. The device of claim 7, wherein the valve opens in response to a command from the controller when a specified condition is detected.
 9. The device of claim 1, wherein the control circuit maintains a cuff pressure between pre-selected pressure

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limits during an ischemic duration of the remote ischemic conditioning treatment protocol.

10. A device for remote ischemic conditioning comprising:

an inflatable cuff configured to encircle a limb of a subject;

a controller removably attached to the cuff, wherein the controller comprises:

a manifold configured to provide fluid communication between the controller and the cuff;

an outlet in fluid communication with the manifold and in removable fluid communication with the inflatable cuff; and

a control circuit configured to implement a remote ischemic conditioning treatment protocol; and

a controller attachment section joined to the cuff, the controller attachment section having a bottom surface that substantially conforms to an outer surface of the cuff, wherein the controller is removably attached to the cuff by selective attachment to the controller attachment section disposed on the cuff;

wherein cuff pressure is controllable by selectively opening a valve of the controller in response to a command from control circuitry of the control circuit;

wherein the controller attachment section provides fluid communication between the controller and a bladder of the cuff via a structure that includes a conduit that has a female section constructed and arranged to mate with the controller outlet and a male section that is constructed and arranged to mate with a valve of the bladder of the cuff; and

wherein the controller outlet has an outer dimension at an end spaced from the controller, and the female section of the conduit has an upper opening that is configured to receive the end of the controller outlet, a cross-sectional size of the upper opening of the female section being greater than the outer dimension of the controller outlet and greater than an inner dimension of the male section.

11. The device of claim 10, further comprising an O-ring seal disposed within the upper opening of the female section, the O-ring seal surrounding and sealing the controller outlet when disposed within the female section.

12. The device of claim 11, wherein a mouth of the upper opening of the female section includes a retaining structure that has an upper surface that forms an acute angle with respect to a direction of elongation of the controller outlet.

13. A device for remote ischemic conditioning comprising:

an inflatable cuff configured to encircle a limb of a subject;

a controller removably attached to the cuff, wherein the controller comprises:

an outlet in removable fluid communication with the inflatable cuff; and

a control circuit configured to implement a remote ischemic conditioning treatment protocol;

wherein cuff pressure is controllable by selectively opening a valve of the controller in response to a command from control circuitry of the control circuit;

wherein fluid communication between the controller and a bladder of the cuff is provided via a structure that includes a conduit that has a female section constructed and arranged to mate with the controller outlet and a male section that is constructed and arranged to mate with a valve of the bladder of the cuff; and

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wherein the controller outlet has an outer dimension at an end spaced from the controller, and the female section of the conduit has an upper opening that is configured to receive the end of the controller outlet, a cross-sectional size of the upper opening of the female section being greater than the outer dimension of the controller outlet.

14. *The device of claim 13, wherein the inflatable cuff comprises:*

at least two flexible sections spaced apart in a longitudinal direction of the cuff and an intermediate section disposed between the two flexible sections, the intermediate section having a greater rigidity than the two flexible sections; and

a plurality of reinforcing structures disposed on at least one of the two flexible sections and being elongated in an axial direction substantially perpendicular to the longitudinal direction of the cuff, wherein when the cuff is inflated, the reinforcing structures distribute pressure applied by the cuff in the axial direction.

15. *The device of claim 14, wherein the plurality of reinforcing structures are spaced apart in a longitudinal direction, and are generally parallel to one another to permit the cuff to bend around an encircled limb while providing increased rigidity in the direction generally perpendicular to the longitudinal direction.*

16. *The device of claim 14, wherein the reinforcing structures are curved.*

17. *The device of claim 14, wherein the reinforcing structures are generally linear.*

18. *The device of claim 14, wherein the reinforcing structures are integrally formed with the flexible sections.*

19. *The device of claim 18, wherein the reinforcing structures comprise portions of the flexible sections which are uncompressed.*

20. *The device of claim 14, wherein the reinforcing structures are formed by providing alternating areas of compressed foam and uncompressed foam.*

21. *The device of claim 14, wherein the reinforcing structures are formed separately from the flexible sections and are attached to at least one of the two flexible sections after formation of the flexible sections.*

22. *The device of claim 14, wherein the reinforcing structures extend substantially across a width of the cuff.*

23. *The device of claim 22, wherein the reinforcing structures distribute pressure applied by the cuff across the width of the cuff in the axial direction.*

24. *The device of claim 14, wherein the reinforcing structures assist in preventing kinks in the cuff assembly.*

25. *The device of claim 14, further comprising: an outer layer; an inner layer; and an inflatable bladder disposed between the inner layer and the outer layer.*

26. *The device of claim 25, wherein the reinforcing structures are formed on the outer layer.*

27. *The device of claim 25, further comprising at least one non-slip structure disposed on an exterior face of the inner layer and configured to face the limb of the subject.*

28. *The device of claim 27, wherein the non-slip structure comprises a strip formed of silicone.*

29. *The device of claim 25, wherein the inner layer is formed of a soft, non-irritating material.*

30. *The device of claim 25, wherein the inner layer is configured to provide moisture absorption, wicking, and/or breathability to the cuff.*

31. *The device of claim 30, wherein the inner layer comprises a cloth material.*

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32. The device of claim 31, wherein the cloth material comprises a felt.

33. The device of claim 25, wherein a fluid inlet to the bladder extends from the bladder through the intermediate section of the outer layer.

34. The device of claim 14, further comprising a fastener to couple together ends of the two flexible sections about the limb of the subject.

35. The device of claim 34, wherein the fastener comprises a hook and loop fastener.

36. The device of claim 14, wherein the intermediate section comprises:

a substantially planar upper surface;

an attachment device configured to removably attach the controller to the upper surface; and
the conduit.

37. The device of claim 36, wherein the intermediate section comprises a curved inner surface extending in the longitudinal direction of the cuff.

38. The device of claim 14, further comprising a controller attachment section disposed on the intermediate section, the controller attachment section being configured to permit removable attachment of the controller.

39. The device of claim 38, wherein the controller attachment section is joined to the intermediate section by two attachment joints that are aligned in a direction generally perpendicular to the longitudinal direction of the cuff.

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40. A device for remote ischemic conditioning comprising:

an inflatable cuff configured to encircle a limb of a subject;

a controller removably attached to the cuff; and

a controller attachment section joined to the cuff, the controller attachment section having a bottom surface that substantially conforms to an outer surface of the cuff, wherein the controller is removably attached to the cuff by selective attachment to the controller attachment section disposed on the cuff, the controller attachment section further comprising:

an upper surface for supporting the controller in an attached state; an upstanding wall surrounding the upper surface; and

a tab mounted at one end of the upper surface and including a projecting edge spaced from the upper surface, the projecting edge facing outwardly toward the upstanding wall;

wherein the controller further comprises a slot that is disposed between a body of the controller and an outer band, and wherein the device is arranged such that when the controller is attached to the controller attachment section, an upper portion of the tab is pushed inwardly away from the outstanding wall so that the tab passes through the slot.

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UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : RE47,219 E
APPLICATION NO. : 15/783628
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INVENTOR(S) : Ganske et al.

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

In the Specification

At Column 1, please replace the heading "RELATED APPLICATIONS," at Line 12 (approx.) and the words "This application," at Line 14 (approx.), with the following:

--*CROSS REFERENCE TO RELATED APPLICATIONS*

NOTICE: More than one reissue application has been filed for the reissue of U.S. Patent No. 9,205,019 B2. The reissue applications are U.S. Reissue Patent Application Serial No. 16/180,644, filed on November 5, 2018, now abandoned, which is a divisional reissue application of U.S. Reissue Patent Application Serial No. 15/783,628 (the present application), filed on October 13, 2017, now U.S. Reissue Patent No. RE47,219 E, issued February 5, 2019, which is a reissue application of U.S. Patent Application Serial No. 14/302,624, filed on June 12, 2014, now U.S. Patent No. 9,205,019 B2, issued December 8, 2015, which--

Signed and Sealed this
Second Day of August, 2022
Katherine Kelly Vidal

Katherine Kelly Vidal
Director of the United States Patent and Trademark Office