

US00RE44476E

(19) **United States**
(12) **Reissued Patent**
Meyers et al.

(10) **Patent Number:** **US RE44,476 E**
(45) **Date of Reissued Patent:** ***Sep. 3, 2013**

(54) **CONSTRAINED PROSTHETIC KNEE WITH
ROTATING BEARING**

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(*) Notice: This patent is subject to a terminal dis-
claimer.

(21) Appl. No.: **12/776,224**

(22) Filed: **May 7, 2010**

Related U.S. Patent Documents

Reissue of:

(64) Patent No.: **6,773,461**
Issued: **Aug. 10, 2004**
Appl. No.: **10/234,362**
Filed: **Sep. 4, 2002**

U.S. Applications:

(63) Continuation of application No. 09/771,061, filed on
Jan. 29, 2001, now Pat. No. 6,485,519.

(51) **Int. Cl.**
A61F 2/38 (2006.01)

(52) **U.S. Cl.**
USPC **623/20.24**; 623/18.11; 623/20.15;
623/20.27; 623/20.28

(58) **Field of Classification Search**
USPC 623/20.15, 20.24, 20.25, 20.26, 20.27,
623/20.28, 20.29, 20.31, 20.33, 20.35
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

1,504,903 A 8/1924 Rowley
2,183,076 A 12/1939 Kaiser

(Continued)

FOREIGN PATENT DOCUMENTS

CA 1073151 3/1980
DE 2 122 390 1/1973

(Continued)

OTHER PUBLICATIONS

Machine generated translation of DE 2 154 338 (published on May
17, 1973).*

(Continued)

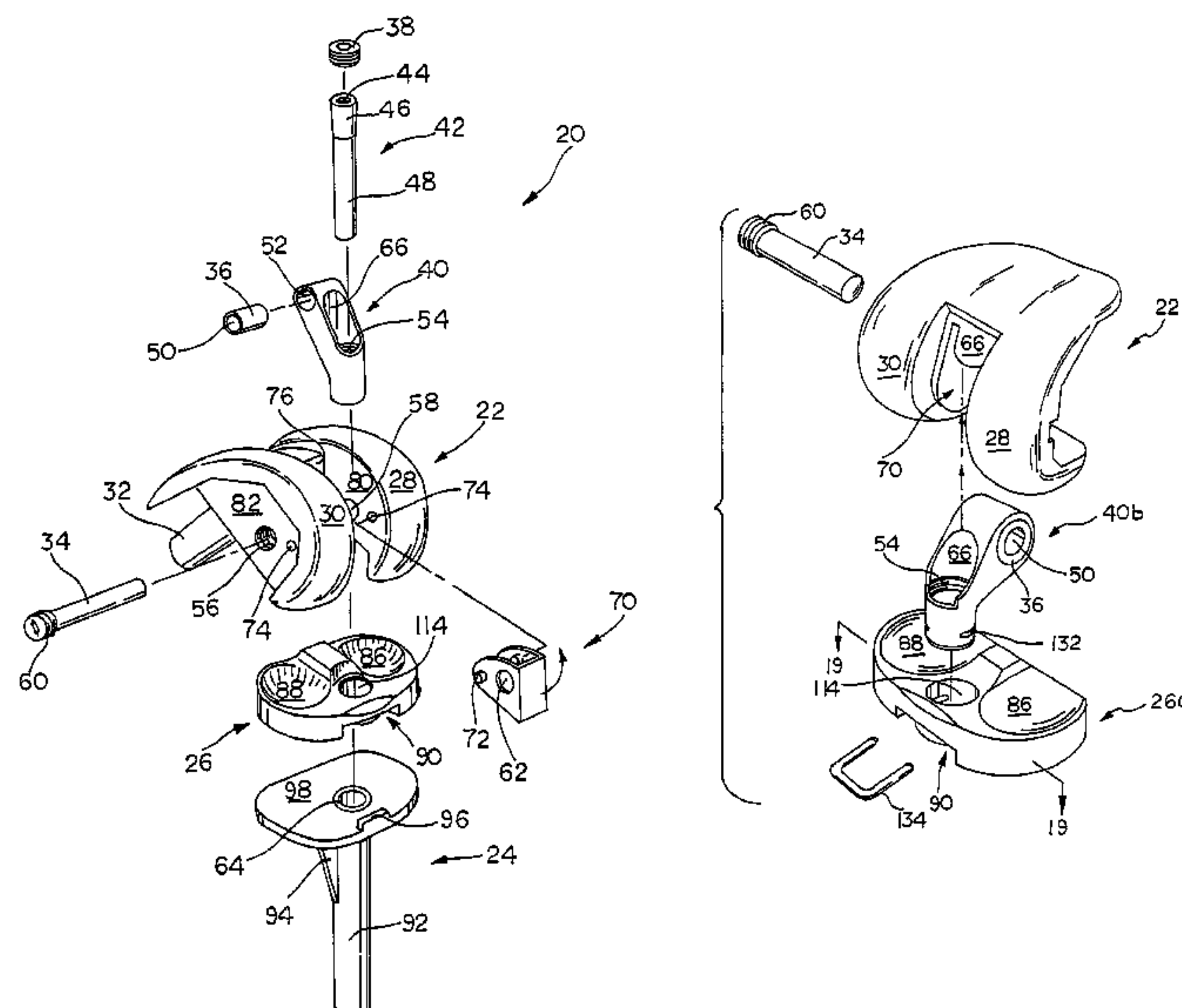
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(57) **ABSTRACT**

A constrained prosthetic knee having a modular hinge post and a rotating bearing. A cannulated hinge post is rotatably connected to the femoral component of the knee prosthesis so that a hinge post extension may be anteriorly positioned through the hinge post and into the tibial component of the knee prosthesis, after positioning of the femoral component in the femur and the tibial component in the tibia. The hinge post is preassembled to the femoral component so that such assembly is not required during the implantation procedure. A meniscal component forming the rotating bearing of the knee prosthesis is packaged together with the hinge post extension so that the appropriate hinge post extension is readily available.

19 Claims, 9 Drawing Sheets



(56)

References Cited

U.S. PATENT DOCUMENTS

3,696,446 A	10/1972	Bousquet et al.	5,413,607 A	5/1995	Engelbrecht et al.
3,708,805 A	1/1973	Scales et al.	5,427,586 A	6/1995	Schelhas
3,813,700 A	6/1974	Tavernetti et al.	5,458,644 A	10/1995	Grunde
3,816,853 A	6/1974	Elson	5,489,307 A	2/1996	Kuslich et al.
3,824,630 A	7/1974	Johnston	5,489,311 A	2/1996	Cipolletti
3,837,009 A	9/1974	Walker	5,549,687 A	8/1996	Coates et al.
3,869,729 A	3/1975	Attenborough	5,549,689 A	8/1996	Epstein et al.
3,909,854 A	10/1975	Martinez	5,609,639 A	3/1997	Walker
3,918,101 A	11/1975	LaGrange et al.	5,609,643 A	3/1997	Colleran et al.
3,924,277 A	12/1975	Freeman et al.	5,658,342 A	8/1997	Draganich et al.
3,934,272 A	1/1976	Wearne et al.	5,683,468 A	11/1997	Pappas
3,996,624 A	12/1976	Noiles	5,702,458 A	12/1997	Burstein et al.
4,016,606 A	4/1977	Murray et al.	5,702,466 A	12/1997	Pappas et al.
4,064,568 A	12/1977	Grunde	5,725,580 A	3/1998	Cloutier et al.
4,092,740 A	6/1978	Eshriqui	5,755,804 A	5/1998	Schmotzer et al.
4,094,017 A	6/1978	Matthews et al.	5,766,257 A	6/1998	Goodman et al.
4,112,522 A	9/1978	Dadurian et al.	5,772,661 A	6/1998	Michelson
4,134,158 A	1/1979	Laure	5,776,200 A	7/1998	Johnson et al.
4,136,405 A	1/1979	Patrick et al.	5,776,201 A	7/1998	Colleran et al.
4,215,439 A	8/1980	Gold	5,800,552 A	9/1998	Forte
4,216,549 A	8/1980	Hillberry et al.	5,824,096 A	10/1998	Pappas et al.
4,219,893 A	9/1980	Noiles	5,824,102 A	10/1998	Buscayret
4,224,697 A	9/1980	Murray	5,879,392 A	3/1999	McMinn
4,257,129 A	3/1981	Volz	5,879,394 A	3/1999	Ashby et al.
4,262,368 A	4/1981	Lacey	5,906,643 A	5/1999	Walker
4,268,920 A	5/1981	Engelbrecht	5,954,770 A	9/1999	Schmotzer et al.
4,301,553 A	11/1981	Noiles	5,964,808 A	10/1999	Blaha et al.
4,340,978 A	7/1982	Buechel et al.	6,004,352 A	12/1999	Buni
4,358,859 A	11/1982	Schurman et al.	6,013,103 A	1/2000	Kaufman et al.
4,383,337 A	5/1983	Volz et al.	6,019,794 A	2/2000	Walker
4,404,691 A	9/1983	Buning	6,080,195 A	6/2000	Colleran et al.
4,462,120 A	7/1984	Rambert et al.	6,099,570 A	8/2000	Livet et al.
4,538,305 A	9/1985	Engelbrecht	6,099,571 A	8/2000	Knapp
4,578,081 A	3/1986	Harder et al.	6,117,175 A	9/2000	Bosredon
4,655,778 A	4/1987	Koeneman	6,126,692 A	10/2000	Robie et al.
4,662,889 A	5/1987	Zichner et al.	6,143,034 A	11/2000	Burrows
4,764,171 A	8/1988	Harder et al.	6,162,255 A	12/2000	Oyola
4,790,853 A	12/1988	Engelbrecht et al.	6,171,342 B1	1/2001	O'Neil et al.
4,790,854 A	12/1988	Harder et al.	6,264,696 B1	7/2001	Reigner et al.
4,822,366 A	4/1989	Bolesky	6,267,763 B1	7/2001	Castro
4,828,564 A	5/1989	Scales et al.	6,296,666 B1	10/2001	Gardner
4,834,758 A	5/1989	Lane et al.	6,306,171 B1	10/2001	Conzemius
4,865,606 A	9/1989	Rehder	6,306,172 B1	10/2001	O'Neil et al.
4,888,021 A	12/1989	Forte et al.	6,319,283 B1	11/2001	Insall et al.
4,919,660 A	4/1990	Peilloud	6,361,564 B1	3/2002	Marceaux et al.
4,923,472 A	5/1990	Ugolini	6,428,577 B1	8/2002	Evans et al.
4,936,853 A	6/1990	Fabian et al.	6,436,145 B1	8/2002	Miller
4,938,769 A	7/1990	Shaw	6,443,991 B1	9/2002	Running
4,944,757 A	7/1990	Martinez et al.	6,447,549 B1	9/2002	Taft
4,950,298 A	8/1990	Custilo et al.	6,485,519 B2	11/2002	Meyers et al.
5,007,933 A	4/1991	Sidebotham et al.	6,491,726 B2	12/2002	Pappas
5,011,496 A	4/1991	Forte et al.	6,500,208 B1	12/2002	Metzger et al.
5,015,255 A	5/1991	Kuslich	6,506,215 B1	1/2003	Letot et al.
5,019,103 A	5/1991	Van Zile et al.	6,620,198 B2	9/2003	Burstein et al.
5,037,439 A	8/1991	Albrektsson et al.	6,629,999 B1	10/2003	Serafin, Jr.
5,061,271 A	10/1991	Van Zile	6,652,588 B2	11/2003	Hayes et al.
5,116,375 A	5/1992	Hofmann	6,719,800 B2	4/2004	Meyers et al.
5,123,928 A	6/1992	Moser	6,743,258 B1	6/2004	Keller
5,139,521 A	8/1992	Schelhas	6,755,864 B1	6/2004	Brack et al.
5,171,283 A	12/1992	Pappas et al.	6,770,097 B2	8/2004	Leclercq
5,180,383 A	1/1993	Haydon	6,773,461 B2	8/2004	Meyers et al.
5,194,066 A	3/1993	Van Zile	6,984,249 B2	1/2006	Keller
5,246,459 A	9/1993	Elias et al.	7,070,622 B1	7/2006	Brown et al.
5,282,867 A	2/1994	Mikhail	7,172,628 B2	2/2007	Lambrich et al.
5,290,313 A	3/1994	Heldreth	7,175,665 B2	2/2007	German et al.
5,314,481 A	5/1994	Bianco	7,232,465 B2	6/2007	Keller
5,326,368 A	7/1994	Collazo	7,326,252 B2	2/2008	Otto et al.
5,330,534 A	7/1994	Herrington et al.	7,357,817 B2	4/2008	D'Alessio, II
5,358,527 A	10/1994	Forte	7,569,054 B2	8/2009	Michelson
5,370,700 A	12/1994	Sarkisian et al.	7,572,292 B2	8/2009	Crabtree et al.
5,370,701 A	12/1994	Finn	7,591,855 B2	9/2009	Keller
5,387,240 A	2/1995	Pottenger et al.	7,658,767 B2	2/2010	Wyss
5,395,401 A	3/1995	Bahler	7,753,960 B2	7/2010	Cipolletti et al.
5,405,398 A	4/1995	Buford, III et al.	7,871,442 B2	1/2011	Servidio
5,411,555 A	5/1995	Nieder	8,268,006 B2	9/2012	Meyers et al.
			2001/0003803 A1	6/2001	LeClercq
			2001/0025199 A1	9/2001	Rauscher
			2001/0034554 A1	10/2001	Pappas
			2002/0103541 A1	8/2002	Meyers et al.

2002/0107576	A1	8/2002	Meyers et al.	EP	0812582	A2	12/1997
2002/0161448	A1	10/2002	Hayes et al.	EP	0 653 194	B1 *	3/1999
2003/0009228	A1	1/2003	Meyers et al.	EP	0923916	A1	6/1999
2003/0009232	A1	1/2003	Metzger et al.	EP	1108403	A1	6/2001
2003/0153980	A1	8/2003	Brack	EP	1132064	A2	9/2001
2004/0054416	A1	3/2004	Wyss et al.	EP	1 226 800	A3	7/2002
2004/0162620	A1	8/2004	Wyss	EP	1226800	A2	7/2002
2004/0186583	A1	9/2004	Keller	EP	1417938	A1	5/2004
2004/0186584	A1	9/2004	Keller	EP	1447060	A2	8/2004
2004/0220676	A1	11/2004	Keller	EP	1447060	A3	3/2006
2004/0249467	A1	12/2004	Meyers et al.	FR	2445137	A1	7/1980
2005/0107886	A1	5/2005	Crabtree et al.	FR	2601873	A1	1/1988
2005/0192672	A1	9/2005	Wyss et al.	FR	2612767	A1	9/1988
2005/0246028	A1	11/2005	Pappas et al.	FR	2628316	A1	9/1989
2007/0100463	A1	5/2007	Aram et al.	FR	2641966	A1	7/1990
2008/0004708	A1	1/2008	Wyss	FR	2692475	A1	12/1993
2008/0097616	A1	4/2008	Meyers et al.	FR	2696926	A1	4/1994
2008/0167722	A1	7/2008	Metzger et al.	FR	2 702 651	A	9/1994
2008/0255671	A1	10/2008	Kriek	FR	2702651	A1	9/1994
2009/0024221	A1	1/2009	Ball	FR	2711750	A1	5/1995
2009/0082873	A1	3/2009	Hazebrouck et al.	FR	2751204	A1	1/1998
2009/0088860	A1	4/2009	Romeis et al.	FR	2760352	A1	9/1998
2009/0125116	A1	5/2009	Crabtree et al.	FR	2771283	A1	5/1999
2009/0149964	A1	6/2009	May et al.	FR	2777453	A1	10/1999
2009/0299482	A1	12/2009	Metzger et al.	FR	2787992	A1	7/2000
2009/0326665	A1	12/2009	Wyss et al.	FR	2793676	A1	11/2000
2009/0326666	A1	12/2009	Wyss et al.	FR	2793677	A1	11/2000
2010/0016978	A1	1/2010	Williams et al.	GB	1328497	A	8/1973
2010/0016980	A1	1/2010	Donno et al.	GB	1409150	A	10/1975
2010/0042224	A1	2/2010	Otto et al.	GB	1457147	A	12/1976
2010/0063594	A1	3/2010	Hazebrouck et al.	GB	1475688	A	6/1977
2010/0100189	A1	4/2010	Metzger	GB	1507309	A	4/1978
2010/0234962	A1	9/2010	Meyers et al.	GB	1509366	A	5/1978

FOREIGN PATENT DOCUMENTS

DE	2122390	A1	1/1973
DE	2154338	A1	5/1973
DE	2810748	A1	11/1978
DE	2906458	A1	8/1979
DE	3013155	A1	10/1980
DE	3039992	A1	5/1981
DE	3339102	A1	5/1984
DE	3529894	A1	3/1987
DE	4102509	A1	7/1992
DE	4110048	C1	7/1992
DE	9414970	U1	12/1994
DE	4434806	A1	4/1996
DE	69206397	T2	8/1996
DE	69305434	T2	11/1997
DE	19809041	A1	9/1999
DE	19915053	A1	10/1999
DE	69324016	T2	10/1999
DE	10012059	A1	9/2001
DE	69712258	T2	3/2003
EP	0 046 926		8/1981
EP	0046926	A2	3/1982
EP	0 069 683	A1	6/1982
EP	0 083 155	A1	11/1982
EP	0069683	A1	1/1983
EP	0083155	A1	7/1983
EP	0 126 978		4/1984
EP	0126978	A1	12/1984
EP	0 194 326	A1	3/1985
EP	0 177 755	A1	9/1985
EP	0 178 445	A1	9/1985
EP	0 194 163	A2	2/1986
EP	0198163	A2	2/1986
EP	0177755	A1	4/1986
EP	0178445	A1	4/1986
EP	0194326	A1	9/1986
EP	0214773	A2	3/1987
EP	0 265 325		4/1988
EP	0265325	A1	4/1988
EP	0177755	B1	11/1988
EP	0410237	A1	1/1991
EP	0420460	A1	4/1991
EP	0472475	A2	2/1992
EP	0716839	A1	6/1996
EP	0724868	A1	8/1996

EP	0812582	A2	12/1997
EP	0 653 194	B1 *	3/1999
EP	0923916	A1	6/1999
EP	1108403	A1	6/2001
EP	1132064	A2	9/2001
EP	1 226 800	A3	7/2002
EP	1226800	A2	7/2002
EP	1417938	A1	5/2004
EP	1447060	A2	8/2004
EP	1447060	A3	3/2006
FR	2445137	A1	7/1980
FR	2601873	A1	1/1988
FR	2612767	A1	9/1988
FR	2628316	A1	9/1989
FR	2641966	A1	7/1990
FR	2692475	A1	12/1993
FR	2696926	A1	4/1994
FR	2 702 651	A	9/1994
FR	2702651	A1	9/1994
FR	2711750	A1	5/1995
FR	2751204	A1	1/1998
FR	2760352	A1	9/1998
FR	2771283	A1	5/1999
FR	2777453	A1	10/1999
FR	2787992	A1	7/2000
FR	2793676	A1	11/2000
FR	2793677	A1	11/2000
GB	1328497	A	8/1973
GB	1409150	A	10/1975
GB	1457147	A	12/1976
GB	1475688	A	6/1977
GB	1507309	A	4/1978
GB	1509366	A	5/1978
GB	1514479	A	6/1978
GB	2070939	A	9/1981
GB	2120943	A	12/1983
GB	2 129 306		5/1984
GB	2129306	A	5/1984
JP	5241775	A	9/1993
JP	8-173464	A	7/1996
JP	10-014935	A	1/1998
RU	2080840	C1	6/1997
WO	WO-8100606	A1	3/1981
WO	WO-8906947	A1	8/1989
WO	WO 94/21198		9/1994
WO	WO00/66043	*	11/2000
WO	WO 00/66043	A1	11/2000
WO	WO-0100606	A1	4/2001

OTHER PUBLICATIONS

The Office Action mailed Dec. 1, 2009 in U.S. Appl. No. 11/956,998.
The European Search Report issued Feb. 3, 2006 in related European Application No. EP04012041.2.
The European Office Action mailed Jul. 3, 2007 in related European Application No. EP04012041.2.
The European Office Action mailed Sep. 26, 2007 in related European Application No. EP03255512.0.
The Canadian Office Action mailed Mar. 2, 2009 in related Canadian Application No. 2,367,652.
The Response filed Sep. 2, 2009 to the Canadian Office Action mailed Mar. 2, 2009 in related Canadian Application No. 2,367,652.
The Office Action mailed Dec. 2, 2010 in U.S. Appl. No. 12/776,218.
The Office Action mailed Nov. 19, 2010 in U.S. Appl. No. 12/776,221.
The Office Action mailed Mar. 3, 2011 in U.S. Appl. No. 12/790,181.
The Amendment filed Apr. 4, 2011 in U.S. Appl. No. 12/776,218.
The Amendment filed Apr. 4, 2011 in U.S. Appl. No. 12/776,221.
The Amendment filed Apr. 4, 2011 in U.S. Appl. No. 12/790,181.
European office action mailed Nov. 2, 2010 in European Patent Application No. 02250512.7.
European Search Report completed Dec. 10, 2010 in European Patent Application No. 10012582.2.
European Search Report completed Dec. 13, 2010 in European Patent Application No. 10012581.4.
The Office Action mailed Apr. 18, 2011 in U.S. Appl. No. 12/776,221.

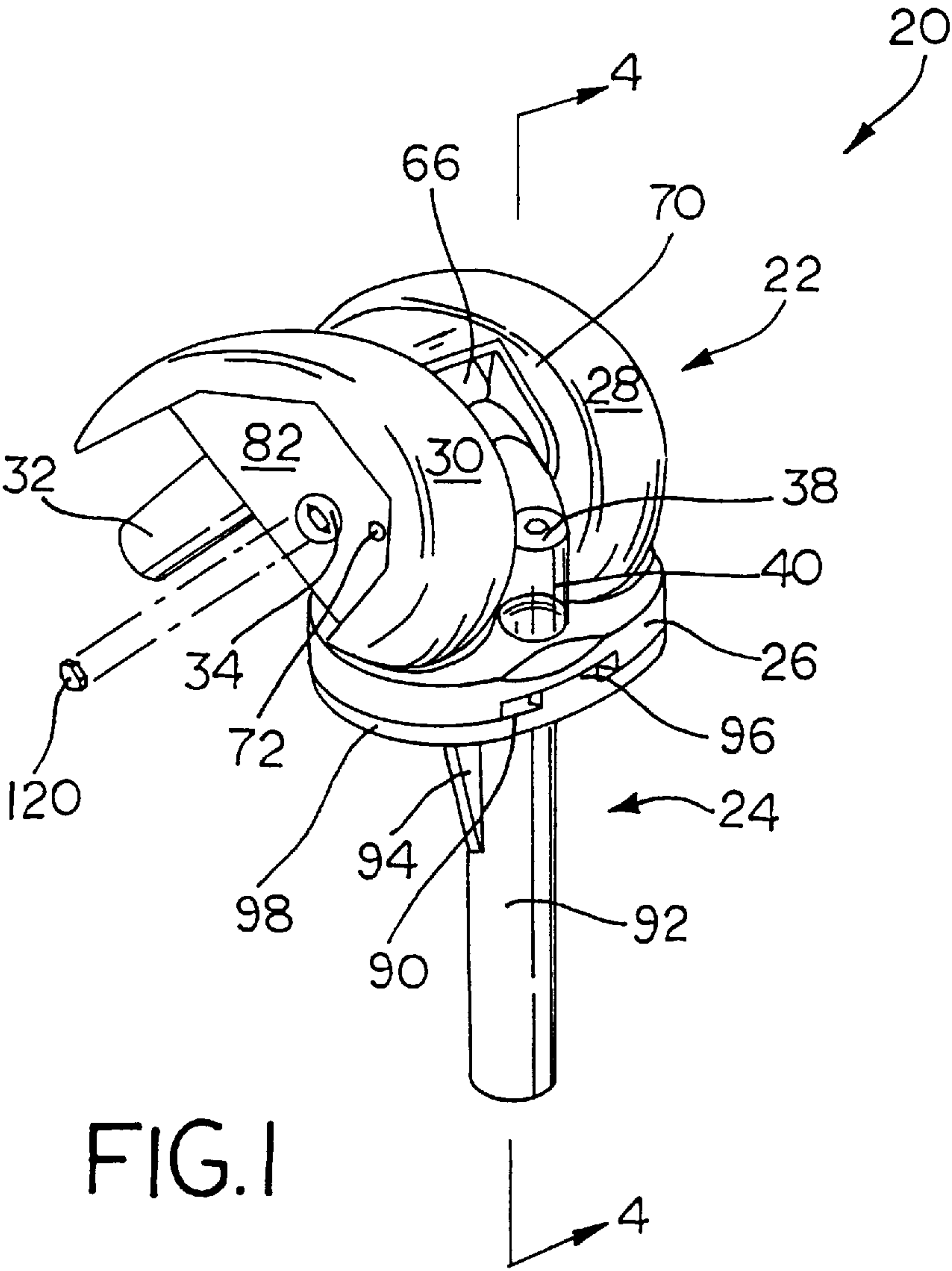
US RE44,476 E

Page 4

The Amendment filed Oct. 18, 2011 in U.S. Appl. No. 12/776,221.
The Office Action mailed Oct. 28, 2011 in U.S. Appl. No. 12/776,221.
The Office Action mailed Apr. 18, 2011 in U.S. Appl. No. 12/776,218.
The Amendment filed Aug. 18, 2011 in U.S. Appl. No. 12/776,218.
The Office Action mailed Sep. 8, 2011 in U.S. Appl. No. 12/776,218.
The Amendment filed Mar. 7, 2012 in U.S. Appl. No. 12/776,218.
The Office Action mailed Feb. 28, 2002 in U.S. Appl. No. 09/771,061.
The Amendment filed May 28, 2002 in U.S. Appl. No. 09/771,061.
The Office Action mailed May 2, 2003 in U.S. Appl. No. 10/001,000.
The Amendment filed Jul. 25, 2003 in U.S. Appl. No. 10/001,000.
The Office Action mailed Jan. 3, 2007 in related Application No. 10/805,056.
The Amendment filed Apr. 3, 2007 in U.S. Appl. No. 10/805,056.
The Office Action mailed Jun. 15, 2007 in U.S. Appl. No. 10/805,056.
The Office Action mailed Dec. 11, 2009 in U.S. Appl. No. 11/956,998.
“U.S. Appl. No. 12/776,218, Final Office Action mailed Apr. 24, 2012”, 9 pgs.
“U.S. Appl. No. 12/776,221, Final Office Action mailed Apr. 12, 2012”, 5 pgs.

“U.S. Appl. No. 12/776,221, Response filed Mar. 28, 2012 to Non Final Office Action mailed Oct. 28, 2011”, 15 pgs.
“U.S. Appl. No. 12/776,221, Response filed Apr. 4, 2011 to Non Final Office Action mailed Nov. 19, 2010”, 14 pgs.
“U.S. Appl. No. 12/790,181, 312 Amendment filed Oct. 19, 2011”, 13 pgs.
“U.S. Appl. No. 12/790,181, Notice of Allowance mailed May 9, 2012”, 7 pgs.
“U.S. Appl. No. 12/790,181, Preliminary Amendment filed Apr. 26, 2012”, 13 pgs.
“U.S. Appl. No. 12/790,181, Preliminary Amendment filed Jul. 15, 2011”, 12 pgs.
“U.S. Appl. No. 12/790,181, PTO Response to 312 Amendment mailed Oct. 31, 2011”, 2 pgs.
“European Application Serial No. 03255512.0, European Search Report mailed Dec. 5, 2004”, 19 pgs.
“European Application Serial No. 04012041.2, European Search Report mailed Mar. 22, 2006”, 24 pgs.
“European Application Serial No. 10012582.2, Amendment filed Sep. 30, 2010”.
“European Application Serial No. 10012582.2, Response filed May 12, 2011 to Search Opinion mailed Dec. 20, 2010”.

* cited by examiner



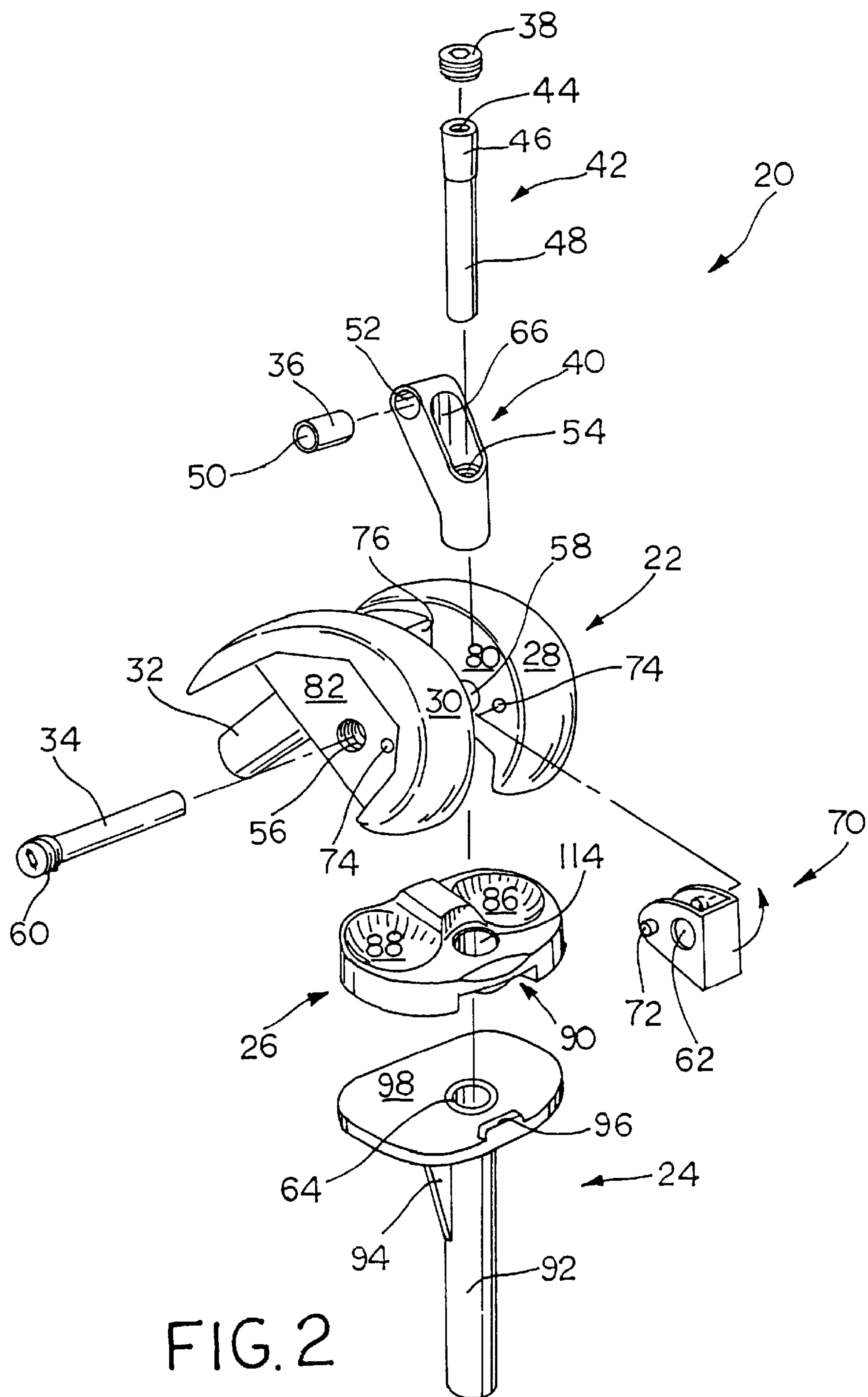
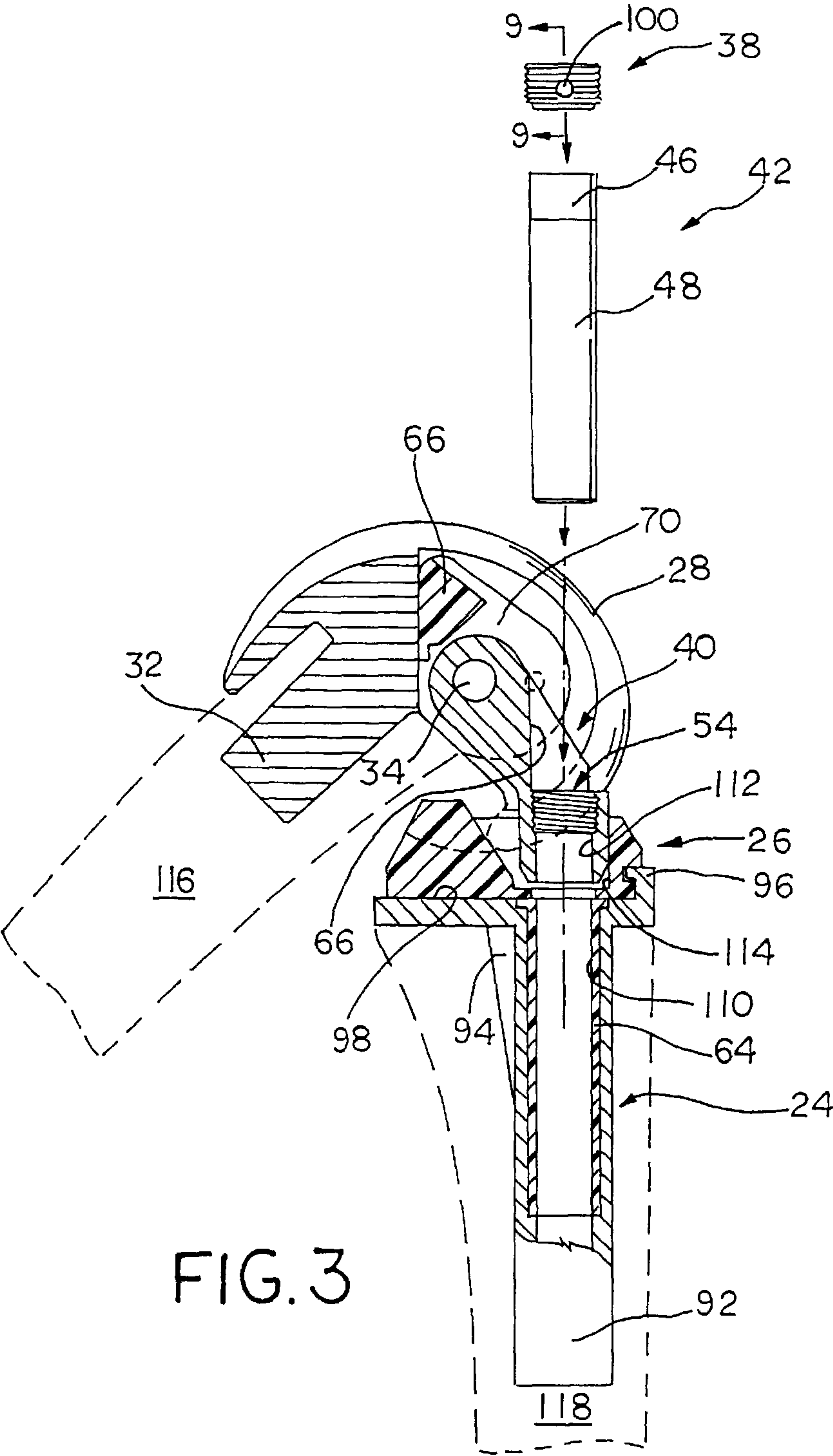


FIG. 2



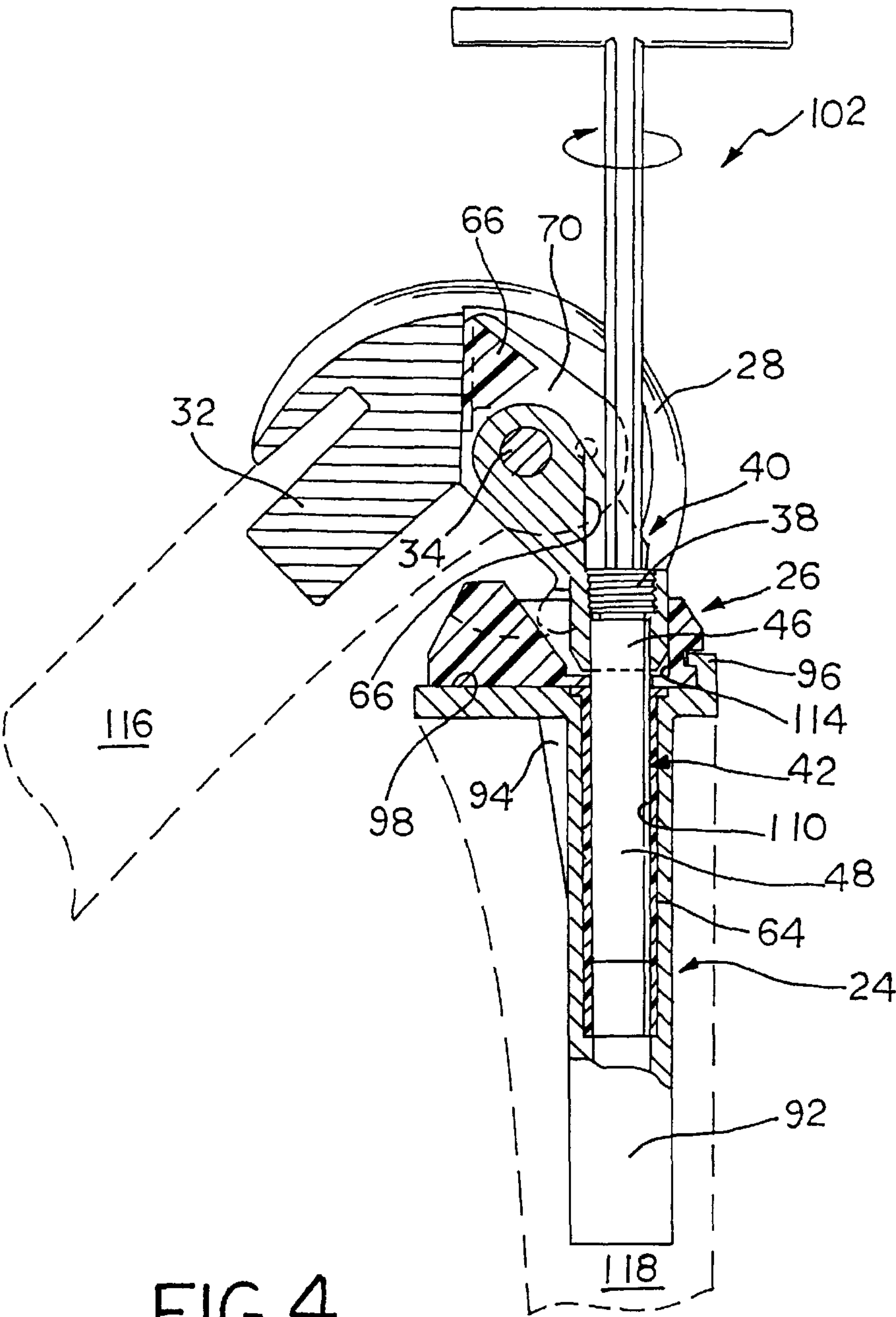
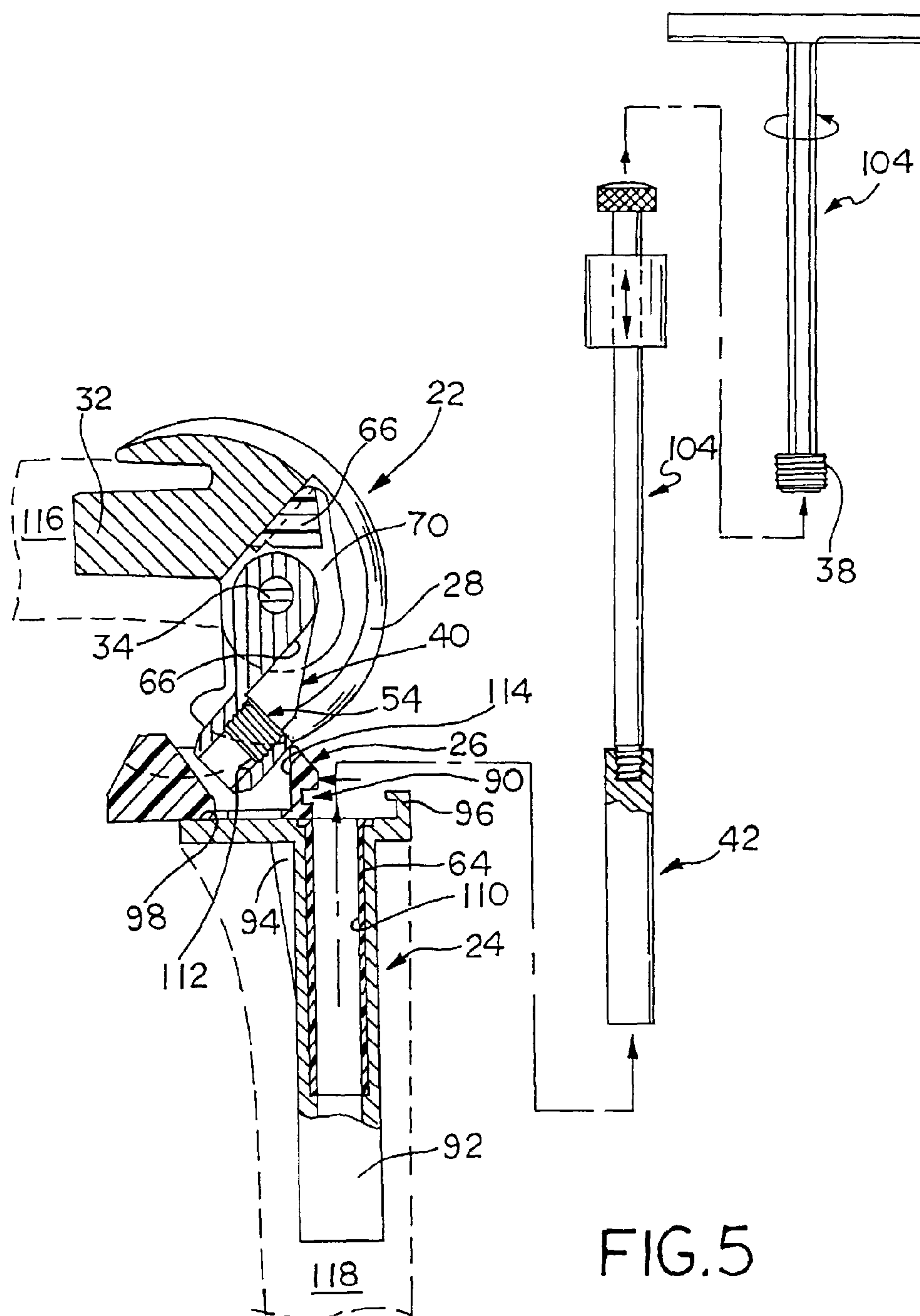


FIG. 4



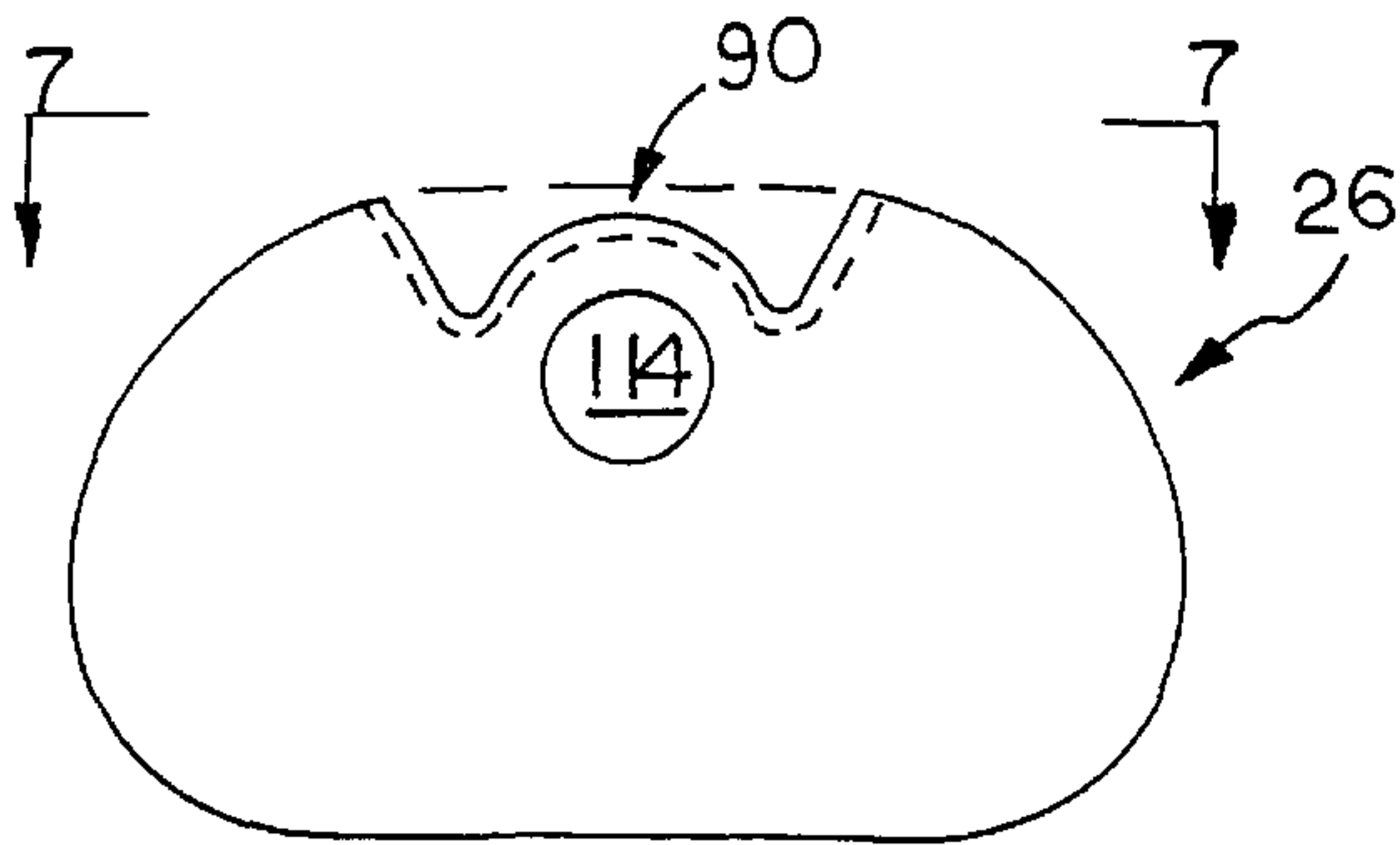


FIG. 6

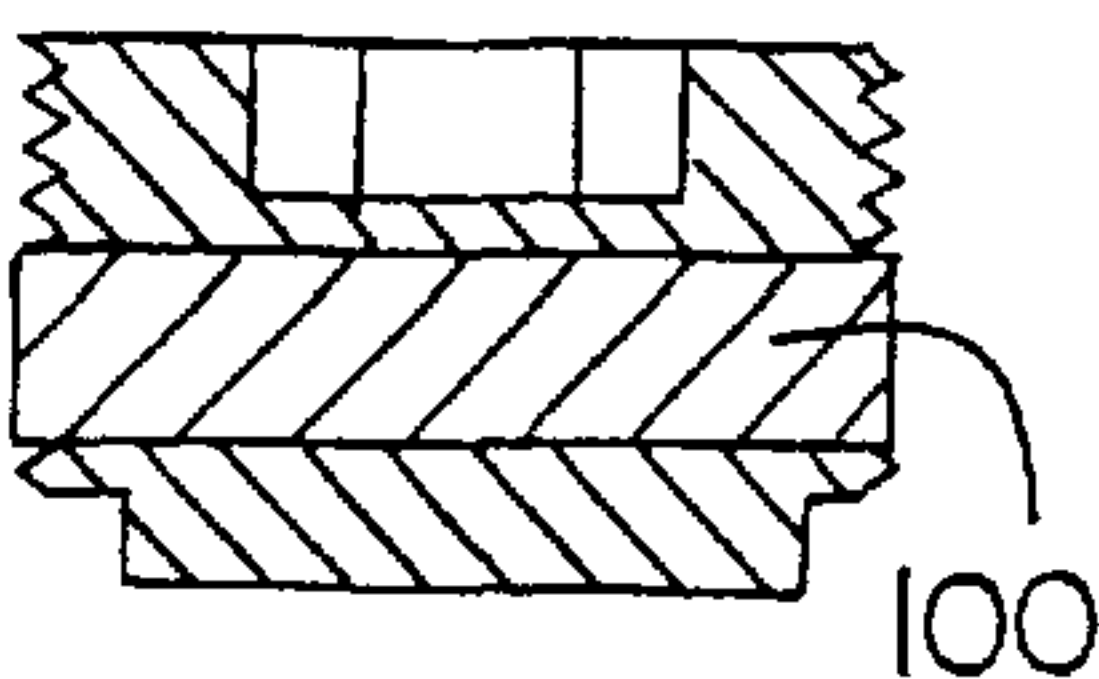


FIG. 9

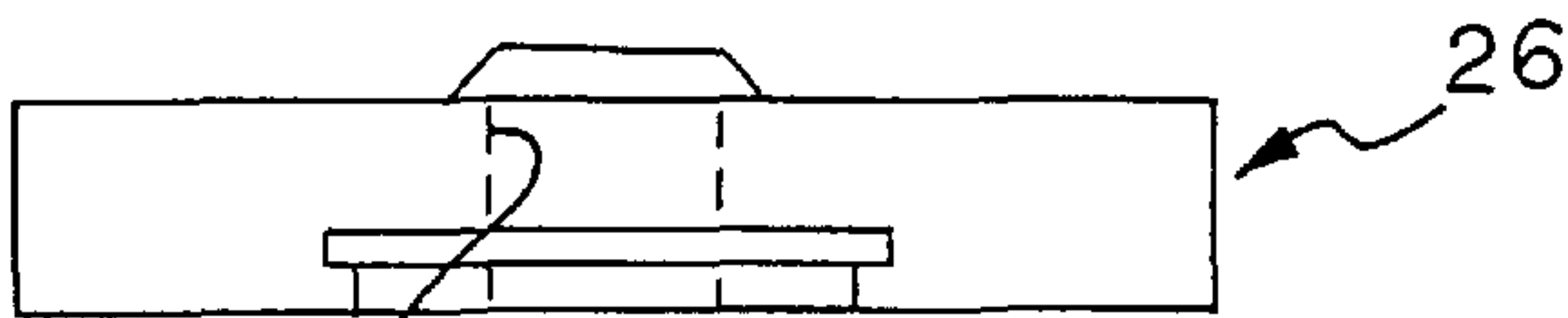


FIG. 7

FIG. 8

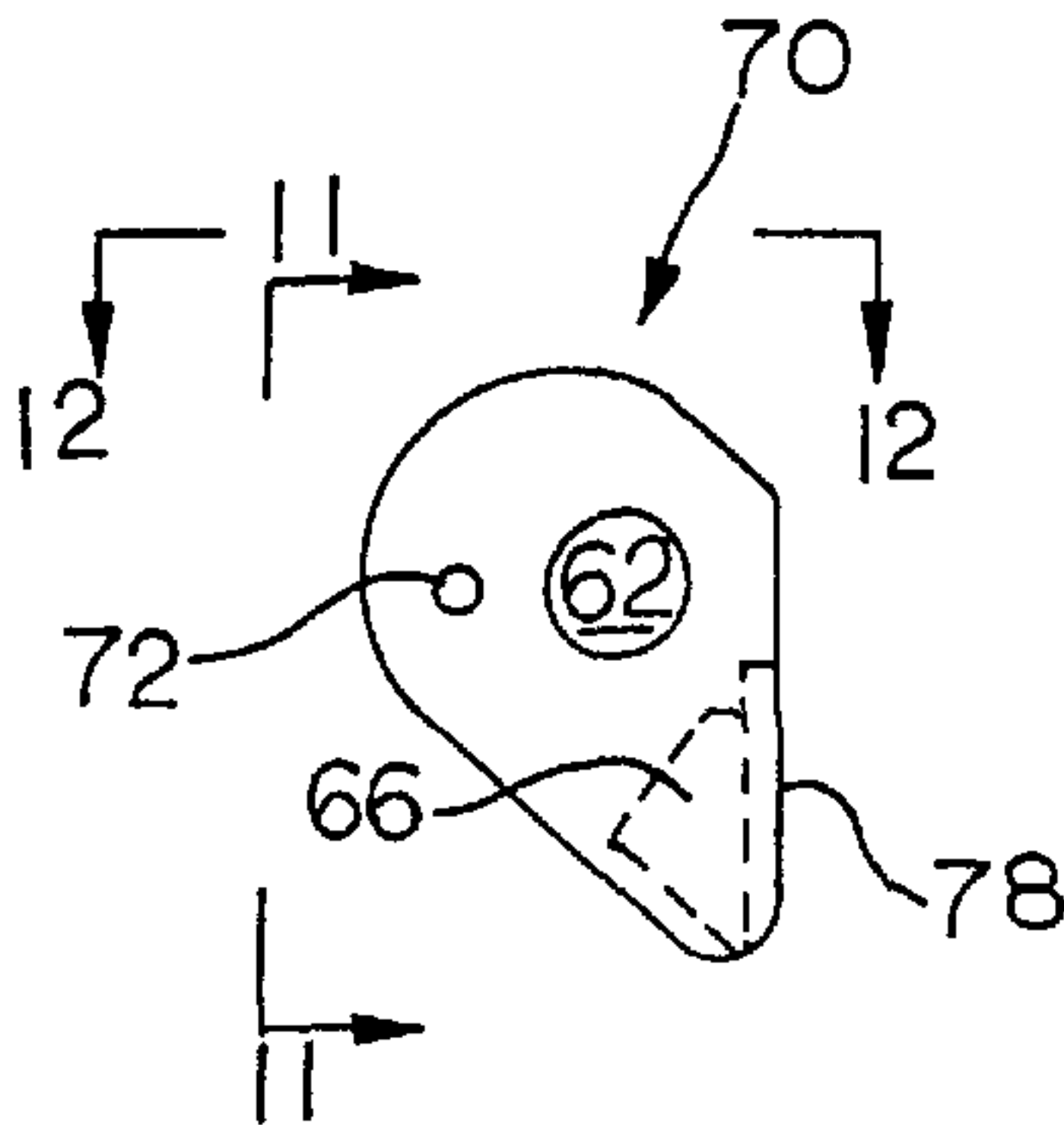
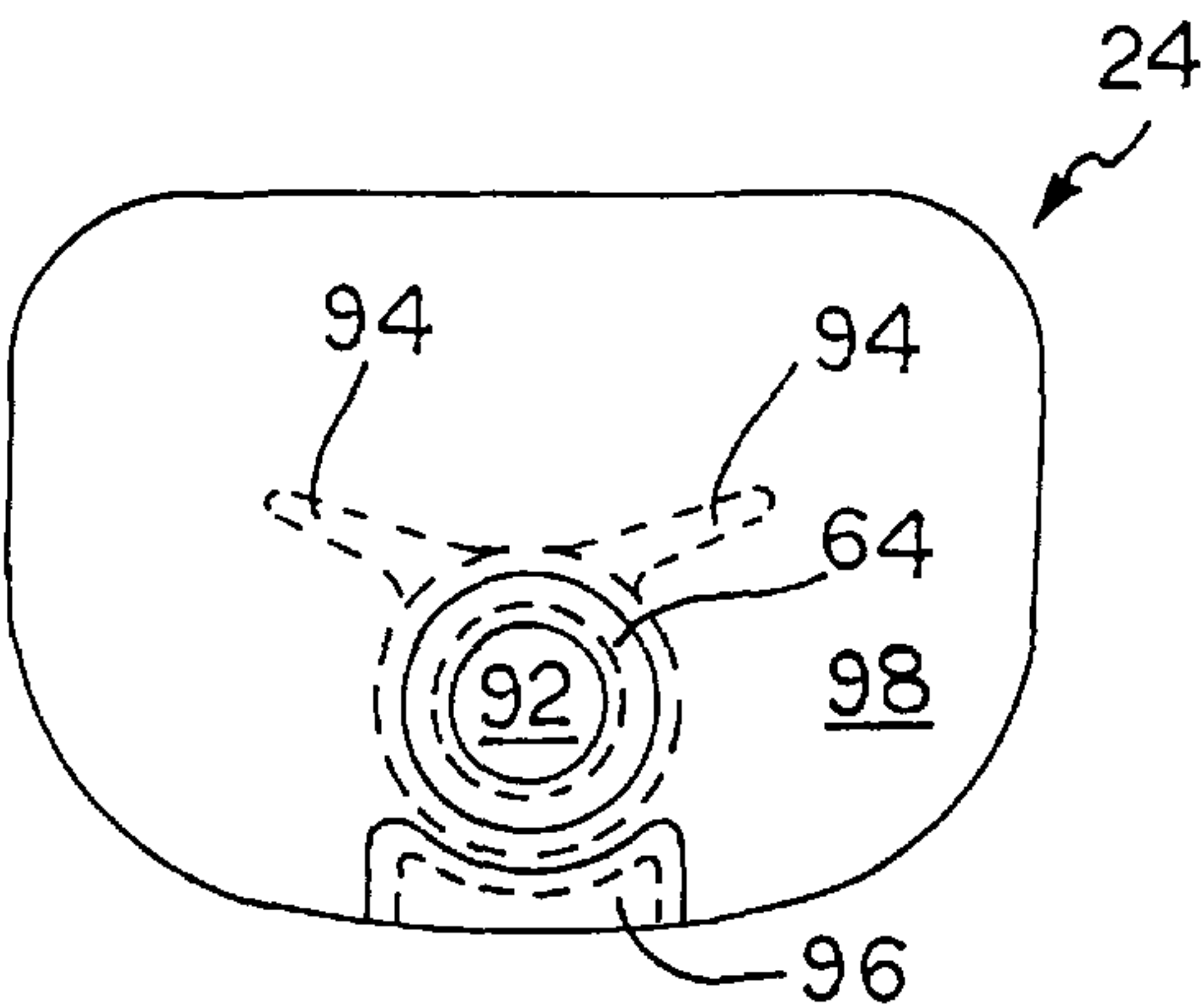


FIG. 10

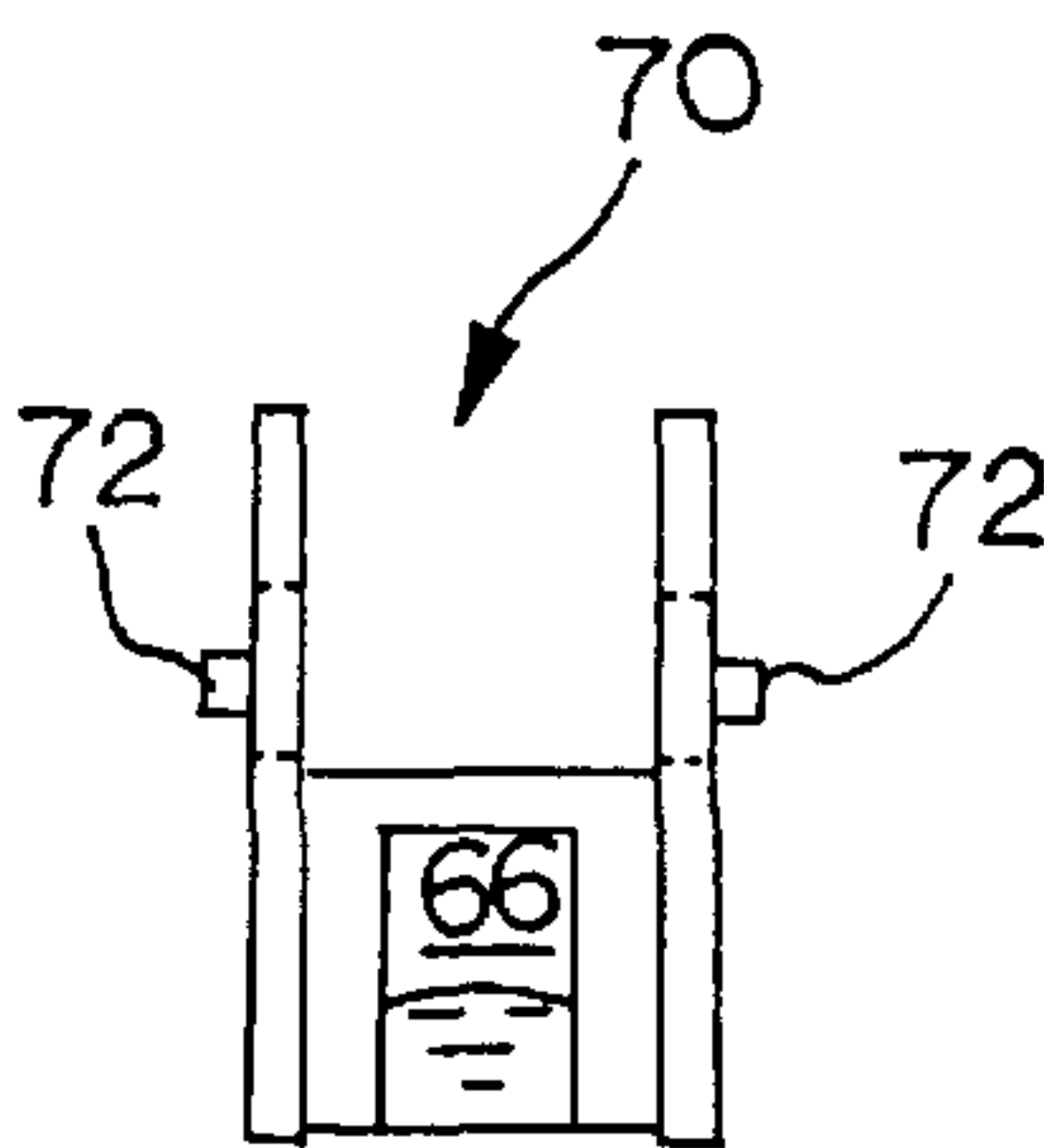


FIG. 11

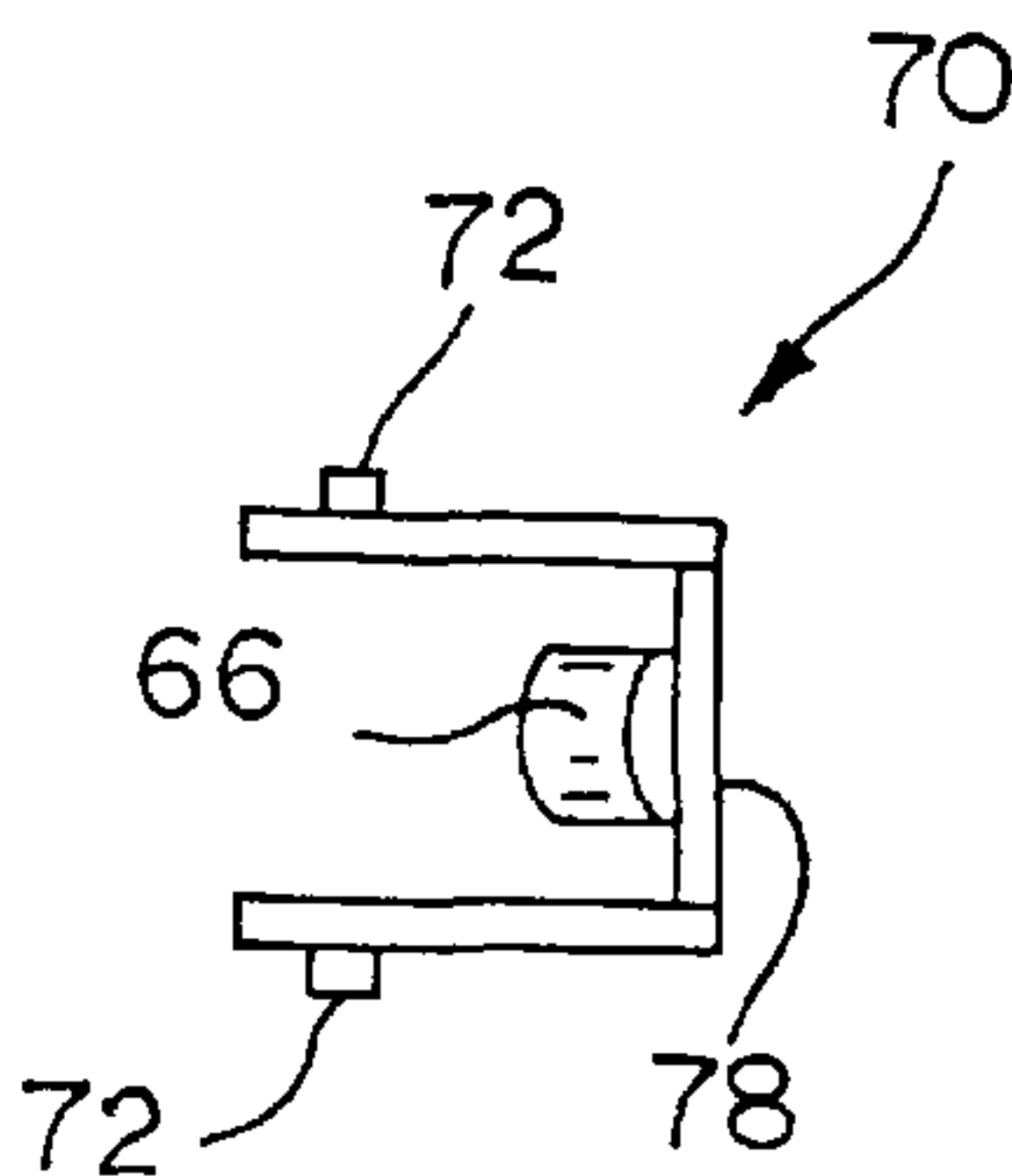
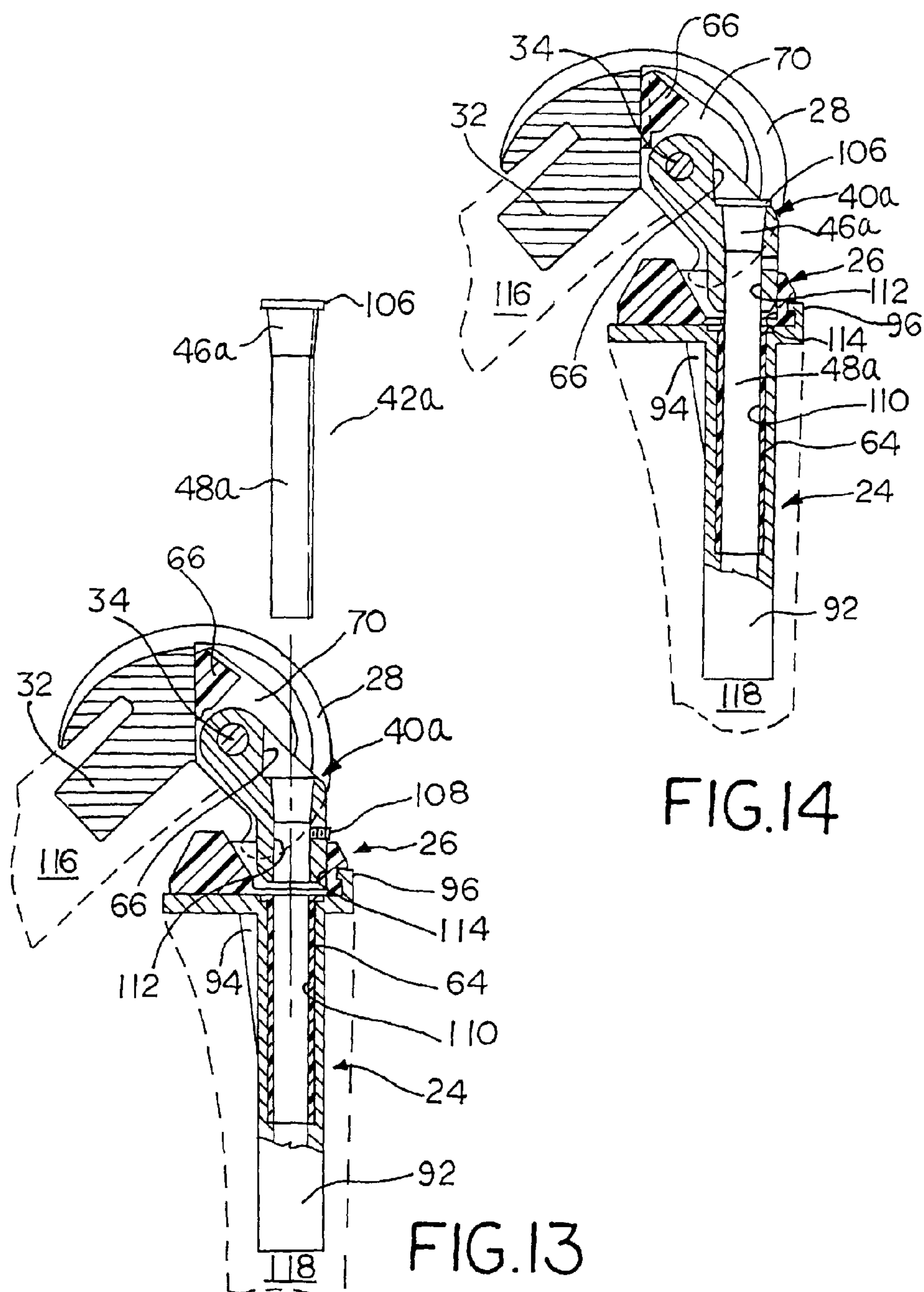


FIG. 12



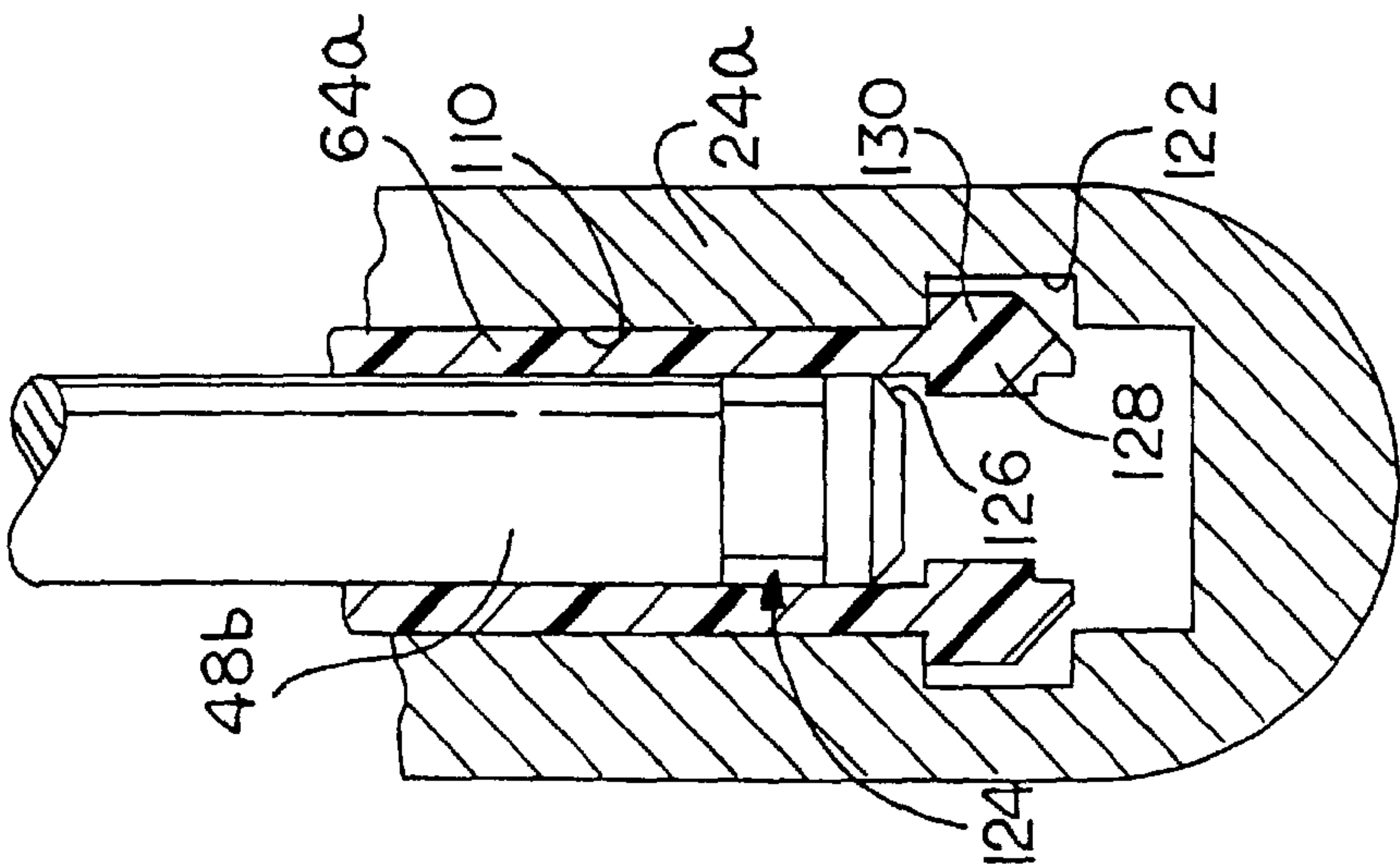


FIG. 15

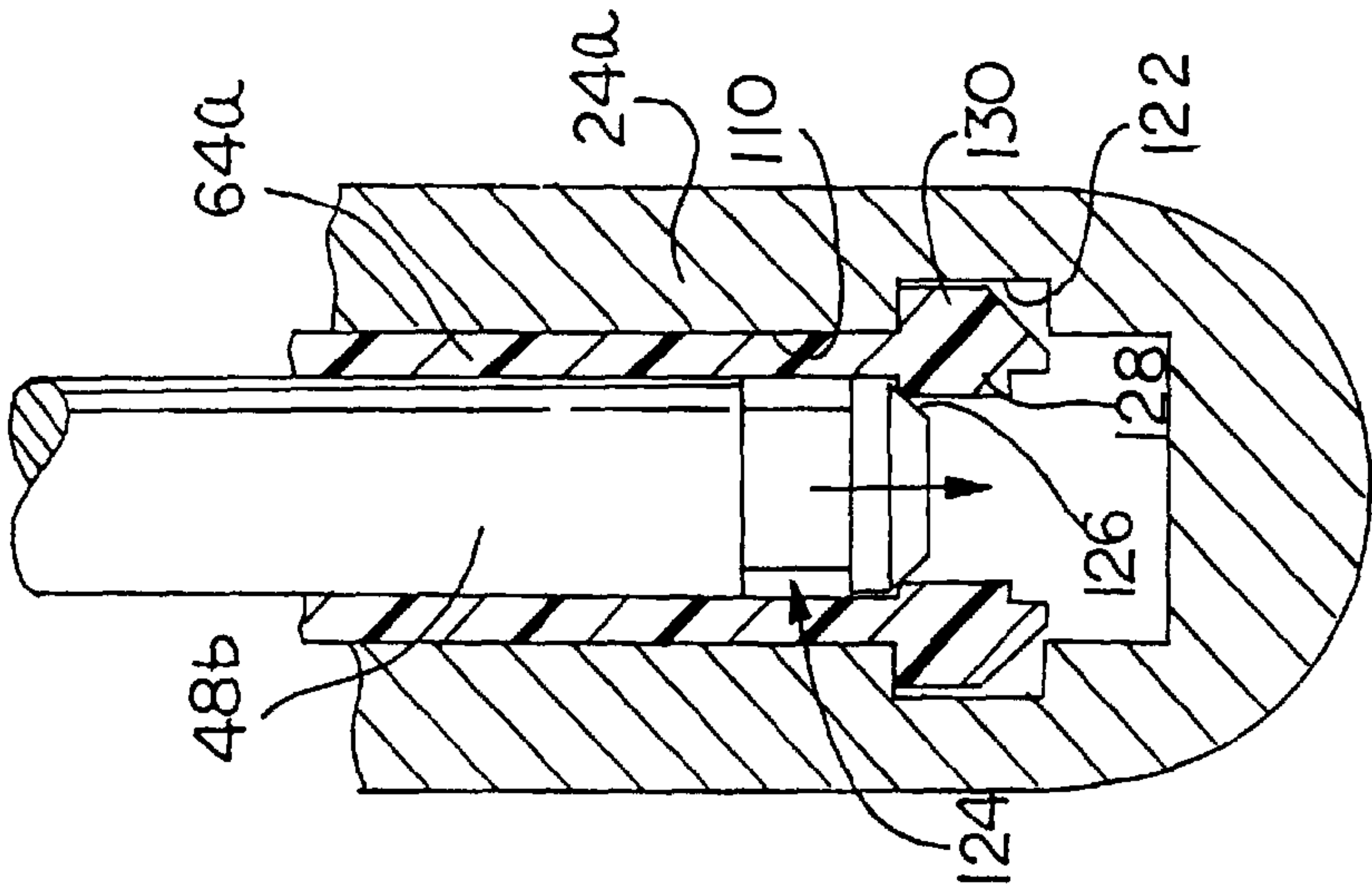


FIG. 16

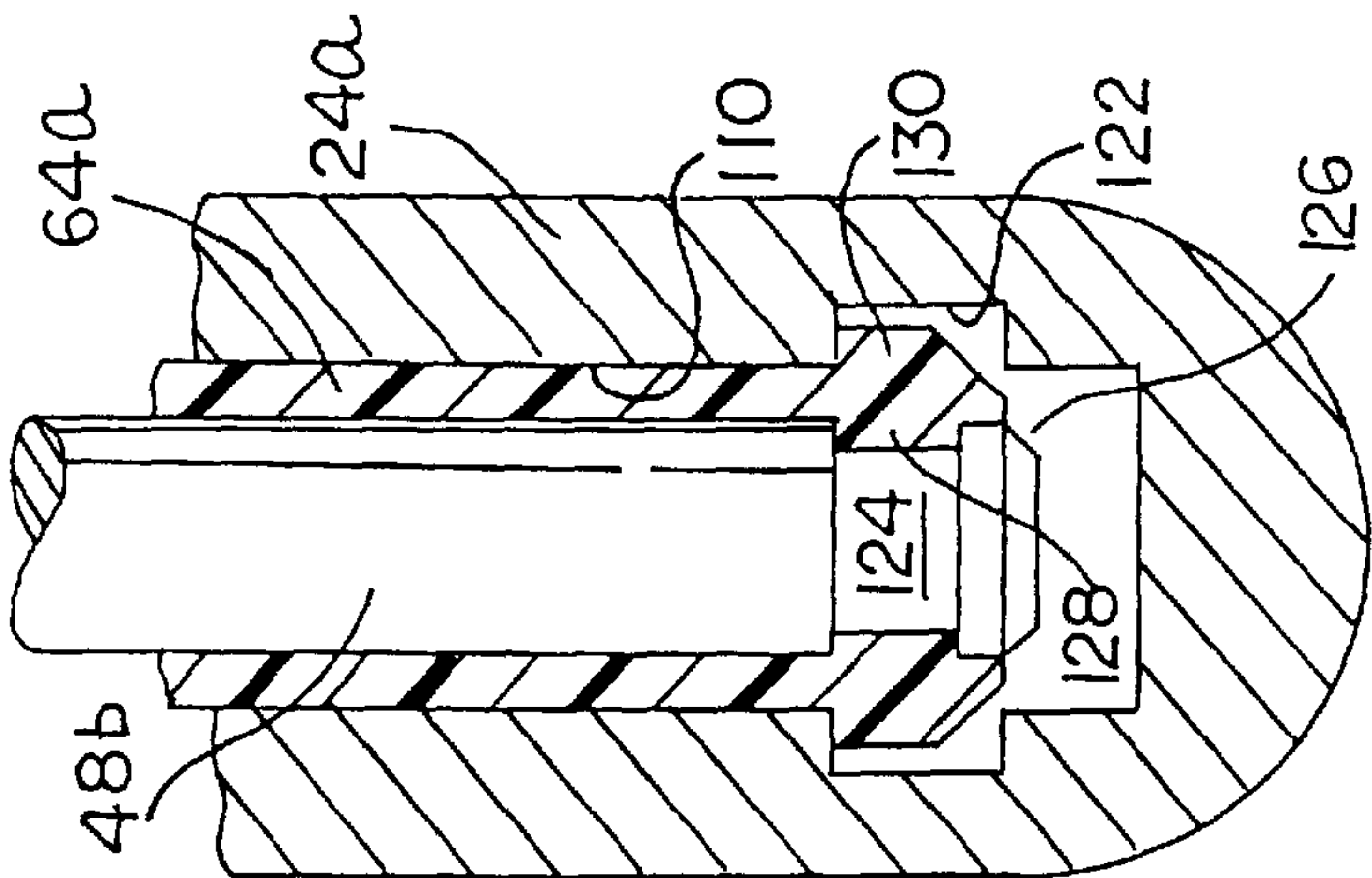
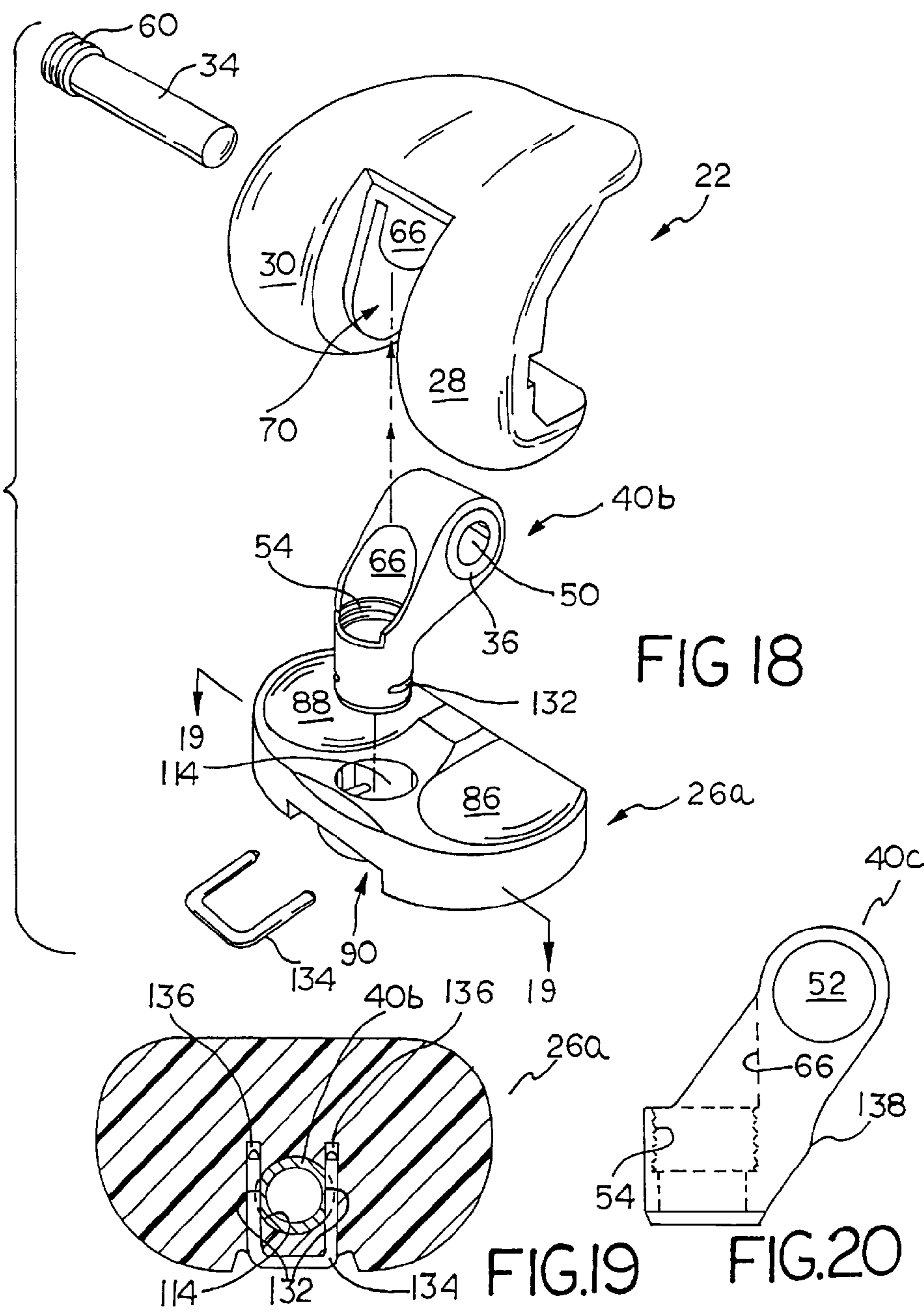


FIG. 17



CONSTRAINED PROSTHETIC KNEE WITH ROTATING BEARING

Matter enclosed in heavy brackets [] appears in the original patent but forms no part of this reissue specification; matter printed in italics indicates the additions made by reissue.

CROSS-REFERENCED TO RELATED APPLICATIONS

This is a continuation of application Ser. No. 09/771,061, filed Jan. 29, 2001, now U.S. Pat. No. 6,485,519.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention relates to prosthetic joints, and, more particularly to a constrained prosthetic knee having a modular hinge post and a rotating bearing.

2. Description of the Related Art

Generally, the knee is formed by the pair of condyles at the distal portion of the femur, the lower surfaces of which bear upon the correspondingly shaped proximal surface plateau of the tibia. The femur and tibia are connected by means of ligaments such as, the posterior cruciate ligament, the lateral collateral ligament, the medial collateral ligament, and the anterior cruciate ligament. These ligaments provide stability to the joint formed by the femur and tibia (i.e., the knee).

In a broad sense, prosthetic knee joints can be considered either constrained or unconstrained. For the purposes of this discussion, constrained prosthetic knees include femoral and tibial prosthetic components which are mechanically linked or constrained to each other by a hinge structure. An unconstrained prosthetic knee includes femoral and tibial components which are not mechanically linked. An unconstrained knee utilizes the patient's existing ligaments to provide joint stability. With this in mind, constrained prosthetic knees have particular applicability to cases in which a patient has experienced ligament loss and/or the existing ligaments do not provide adequate support and stability to the knee.

Tibial components of a prosthetic knee can be formed as a one-piece configuration in which the tibial tray forms the meniscal component of the prosthetic knee. Various other prosthetic knees utilize a modular meniscal component separate from the tibial component. Devices utilizing modular meniscal components include those in which the meniscal component (i.e., tibial bearing surface) is fixed to the tibial tray portion of the tibial component and is incapable of movement relative thereto. Alternative devices utilize a modular meniscal component capable of movement relative to the tibial tray. Devices in which relative rotational movement occurs between the meniscal component and the tibial component are typically referred to as rotating bearing knees. Rotating bearing knees thus allow movement between the bearing (i.e., meniscal component) and the tibial tray, as well as movement between the femoral component and the tibial bearing.

Constrained knees of the prior art include constructions in which a hinge post extension is first positioned within a tibial component (with an end protruding therefrom) and is thereafter connected to the femoral component by positioning the hinge post (rotatably attached to the femoral component) over the top of the protruding end of the hinge post extension and thereafter connecting the hinge post extension to the hinge post, e.g., by threading the hinge post extension into the hinge

post. After making this connection, the meniscal component is thereafter slid into position between the femoral component and the tibial component. Meniscal components utilized with these prior art prosthetic knees were fixed to the tibial component.

The present invention is directed to a constrained knee prosthesis with a rotating bearing. The knee prosthesis of the present invention is structured to facilitate implantation thereof. The present invention is further directed to a prosthetic knee implant set having a plurality of matched modular hinge post and meniscal component pairs.

SUMMARY OF THE INVENTION

The present invention provides an improved constrained knee prosthesis having a cannulated hinge post facilitating implantation of the knee prosthesis in a relatively minimally invasive procedure. The prosthetic knee implant set of the current invention includes a separately packaged femoral component, a separately packaged tibial component, and a third package containing a hinge post extension and the meniscal component. Packaging the individual components of a knee prosthesis in this fashion insures that the appropriate hinge post extension is readily available. A bearing box is interposed between the hinge post and the femoral component. The bearing box includes a hyperextension stop which cooperates with the hinge post to prevent hyperextension of the knee prosthesis. Various structures are utilized to prevent the disengagement of the constrained knee prosthesis of the present invention.

A prosthetic knee constructed in accordance with the present invention includes a femoral component having a pair of condyler surfaces and a hinge post rotatably connected to the femoral component between the condyler surfaces. The hinge post is cannulated and accommodates insertion of a hinge post extension shaft therein. The hinge post and hinge post extension include cooperating locking tapers for locking the hinge post extension to the hinge post. Additionally, the hinge post includes internal threads so that a set screw may be threaded therein to further hold the hinge post extension in place. The tibial component includes a hinge post extension aperture into which the hinge post is seated. The meniscal component similarly includes an aperture to accommodate the hinge post and hinge post extension. The meniscal component of the current invention is free to rotate about the hinge post during flexion and extension of the knee joint.

Having a cannulated hinge post through which a hinge post extension may be anteriorly positioned and secured advantageously allows for a relatively minimally invasive knee replacement procedure.

The present invention advantageously provides a constrained prosthetic knee having a rotating bearing flush with the condyler surfaces of the femoral component.

Another advantage of the present invention is the packaging of the prosthesis components and specifically the packaging of the appropriate hinge post extension together with a meniscal component.

BRIEF DESCRIPTION OF THE DRAWINGS

The above-mentioned and other features and advantages of this invention, and the manner of attaining of them, will become more apparent and the invention itself will be better understood by reference to the following description of an embodiment of the invention taken in conjunction with the accompanying drawings, wherein:

3

FIG. 1 is a perspective view of an assembled knee prosthesis in accordance with the present invention;

FIG. 2 is an exploded view thereof;

FIG. 3 is a cutaway, exploded view illustrating assembly of the knee prosthesis of the current invention including the anterior positioning of the hinge post extension into the hinge post;

FIG. 4 is a cutaway view illustrating securement of the hinge plug (i.e., set screw) in the hinge post to facilitate locking of the hinge post extension therein;

FIG. 5 is a cutaway, exploded view illustrating removal of the hinge post extension;

FIG. 6 is a bottom elevational view of the meniscal component of the present invention;

FIG. 7 is a front elevational view thereof;

FIG. 8 is a top elevational view of a tibial component in accordance with the present invention;

FIG. 9 is a sectional view of a hinge plug in accordance with the present invention;

FIG. 10 is a side elevational view of a bearing box in accordance with the present invention;

FIG. 11 is a front elevational view thereof;

FIG. 12 is a top elevational view thereof;

FIG. 13 is a cutaway, exploded view of an alternative embodiment of the knee prosthesis of the present invention;

FIG. 14 is a cutaway view of an assembled knee prosthesis in accordance with the embodiment illustrated in FIG. 13;

FIG. 15 is a fragmentary, cutaway view of an alternative embodiment of the hinge post extension and tibial bushing of the present invention;

FIG. 16 is a fragmentary, cutaway view of the embodiment of FIG. 15 illustrating insertion of the hinge post extension into the tibial bushing;

FIG. 17 is a fragmentary, cutaway view of the embodiment of FIG. 15 illustrating the hinge post extension fully inserted into the tibial bushing;

FIG. 18 is an exploded view of an alternative embodiment of the knee prosthesis of the current invention;

FIG. 19 is a sectional view of a meniscal component in accordance with an alternative embodiment of the present invention; and

FIG. 20 is an elevational view of a hinge post in accordance with an alternative embodiment of the present invention.

Corresponding reference characters indicate corresponding parts throughout the several views. Although the drawings represent embodiments of the invention, the drawings are not necessarily to scale and certain features may be exaggerated to better illustrate and explain the invention. The exemplifications set out herein illustrate embodiments of the invention, in alternative forms, and such exemplifications are not to be construed as limiting the scope of the invention in any manner.

DETAILED DESCRIPTION

Referring now to the drawings and particularly to FIG. 2, knee prosthesis 20 in accordance with the present invention is illustrated. Knee prosthesis 20 generally includes femoral component 22, tibial component 24, and meniscal component 26. Hinge post 40 is rotatably connected to femoral component 22 and includes elongate hinge post extension aperture 112 (FIGS. 3-6, 13, and 14). Elongate aperture 112 accommodates placement of hinge post extension 42 therein. Hinge post extension 42 thereafter traverses hinge post aperture 114 in meniscal component 26 and hinge post extension aperture 110 (FIGS. 3-6, 13 and 14) in tibial component 24. Elongate hinge post extension aperture 112 of hinge post 40 advantageously

4

allows for anterior placement of hinge post extension 42 during surgical implantation of knee prosthesis 20 of the present invention.

As illustrated in FIG. 2, hinge post extension 42 includes locking taper 46 and cylindrical extension 48. Hinge post extension aperture 112 includes a mating locking taper to cooperate with locking taper 46 and lock hinge post extension 42 to hinge post 40. After positioning of hinge post extension 42 through apertures 112, 114, and 110, hinge plug 38 may be threaded into hinge plug threads 54 in elongate aperture 112 of hinge post 40 (FIG. 4). Hinge plug 38 abuts the end of hinge post extension 42 and thereby facilitates locking of locking taper 46 in elongate aperture 112. In one exemplary embodiment, locking taper 46 comprises a two degree locking taper. When prosthetic knee 20 is assembled as illustrated in FIG. 1, condylar bearing surfaces 28, 30 abut bearing surfaces 86, 88 (see, e.g., FIG. 2) in meniscal component 26.

Hinge post extension 42 is typically formed as a one-piece construction of an inert metal such as, e.g., a cobalt-chromium alloy. Hinge post extension 42 may, however, be constructed of other bio-compatible metals or alloys, such as titanium. Throughout this document reference will be made to various components formed of a cobalt-chromium alloy. Any such component may also be constructed of other bio-compatible metals or alloys such as titanium, as is well-known. As illustrated in FIG. 4, hinge plug wrench 102 is utilized to thread hinge plug 38 into hinge plug threads 54 of hinge post 40. As illustrated in FIG. 9, hinge plug 38 includes locking material 100 to provide a locking connection between hinge plug 38 and hinge plug threads 54 in hinge post 40. Hinge plug 38 is, in one exemplary embodiment formed of a cobalt-chromium alloy. Locking material 100 comprises any suitable biocompatible polymer such as, e.g., ultra-high molecular weight polyethylene (UHMWPE).

As illustrated, e.g., in FIG. 2, femoral component 22 includes condylar bearing surfaces 28, 30 with bearing box wall 76 positioned therebetween. Femoral component 22 further includes external side walls 82, only one of which can be seen in FIG. 2. Condylar bearing surfaces 28, 30 are smooth and highly polished, generally spheroidally shaped and extend outwardly from external side walls 82, as is well known in the industry. Femoral component 22 further includes modular femoral stem 32 for insertion into femur 116 (FIGS. 3-5, 13, and 14), as is known in the art. Femoral component 22 further includes internal side walls 80, only one of which is illustrated in FIG. 2. Internal side walls 80 are substantially perpendicular to bearing box wall 76 and extend outwardly therefrom. Femoral component 22 is typically formed as a one-piece construction of an inert metal such as, e.g., a cobalt-chromium alloy.

Bearing box 70 is designed for placement between condylar bearing surfaces 28, 30 of femoral component 22 as illustrated, e.g., in FIG. 1. Bearing box 70 is further illustrated in FIGS. 10-12 and includes affixing protrusions 72, hinge pin aperture 62, hyperextension stop 66, and anti-rotation surface 78. As illustrated in FIG. 2, femoral component 22 includes affixing protrusion apertures 74 sized to receive affixing protrusions 72. FIG. 1 illustrates bearing box 70 operably positioned on femoral component 22, with anti-rotation surface 78 flush with bearing box wall 76 of femoral component 22, and affixing protrusions 72 received in affixing protrusion apertures 74. The abutting relationship of anti-rotation surface 78 with bearing box wall 76 discourages rotation of bearing box 70 about the longitudinal axis of affixing protrusions 72. When bearing box 70 is positioned on femoral component 22, hinge pin apertures 62 of bearing box 70 align with threaded hinge pin aperture 56 and hinge pin aperture 58

5

of femoral component 22. Bearing box 70 can be formed of any suitable plastic, such as, e.g., UHMWPE.

Hinge post 40 is rotatably connected to femoral component 22 via hinge pin 34. Hinge post 40 is placed between opposing walls of bearing box 70 and is positioned so that hinge pin aperture 52 is aligned with apertures 56, 58, and 62. The opposing walls of bearing box 70 thus act as a bearing surface between hinge post 40 and internal side walls 80 of femoral component 22. Prior to placement of hinge post 40 between opposing walls of bearing box 70, hinge pin sleeve 36 is operably positioned within hinge pin aperture 52 of hinge post 40. Hinge post 40 is formed from a cobalt-chromium alloy, while hinge pin sleeve 36 is formed from a suitable plastic, such as, e.g., UHMWPE. Hinge pin sleeve 36 acts as a bearing between hinge pin aperture 52 of hinge post 40 and hinge pin 34. Accordingly, hinge pin sleeve 36 includes hinge pin aperture 50 sized to accommodate hinge pin 34. After positioning of hinge post 40 between the opposing walls of bearing box 70, hinge pin 34 is positioned through apertures 56, 62, 50, and 58. Hinge pin threads 60 are thereafter threadedly engaged in the threads of threaded hinge pin aperture 56 until the head of hinge pin 34 is flush with external side wall 82.

As illustrated in FIG. 1, hinge pin plug 120 is positioned within the hexagonal indentation of hinge pin 34 after installation of hinge pin 34 as described above. When positioned within the hexagonal indentation of hinge pin 34, hinge pin plug 120 is flush with the head of hinge pin 34. In use, hinge pin plug 120 substantially prohibits the entry of foreign materials into the hexagonal indentation of hinge pin 34. For example, hinge pin plug 120 substantially prohibits bone growth into the hexagonal indentation of hinge pin 34, as well as prohibiting positioning of bone cement therein. The above-described connection of hinge post 40 to femoral component 22 is performed prior to implantation of femoral component 22. Femoral component 22 is packaged and sold with bearing box 70, hinge post 40, hinge pin sleeve 36, hinge pin 34, and hinge pin plug 120 preassembled as described above, with the assembly preferably occurring in the manufacturing environment.

Pre-assembly of hinge post 40 to femoral component 22 eliminates a number of meticulous assembly steps (many of which were performed during implantation) which were required with constrained knees of the prior art. Furthermore, the assembly of hinge post 40 and femoral component 22 as described above facilitates replacement of various portions of knee prosthesis 20. Specifically, the threaded connection of hinge pin 34 to femoral component 22 allows for removal and replacement of various components of knee prosthesis including, e.g., bearing box 70, hinge pin sleeve 36, and hinge post 40.

In use, femoral bone stock may abut external side walls 82 of femoral component 22 and extend to the underside of condylar bearing surfaces 28, 30. To remove hinge pin 34, a hole saw is utilized to remove a relatively small portion of femoral bone stock to provide access to hinge pin 34. Advantageously, femoral component 22 does not require extensive removal of femoral bone stock for implantation thereof (since bone stock can extend to the underside of condylar bearing surfaces 28, 30), and, furthermore, does not require removal of femoral component 22 to effect replacement of, e.g., hinge post 40, bearing box 70, or hinge pin sleeve 36. Upon accessing hinge pin 34 (e.g., utilizing a hole saw as described above), hinge pin plug 120 is removed, e.g., with a scalpel and forceps to provide access to the hexagonal indentation of hinge pin 34 so that a hexagonal wrench may be inserted therein to unthread hinge pin 34 from femoral component 22.

6

Knee prosthesis 20 includes a pair of hyperextension stop mechanisms. The first hyperextension stop comprises a portion of condylar bearing surfaces 28, 30 of increased radius of curvature as compared to the remaining condylar bearing surface. At three degrees of hyperextension this portion of increased radius of curvature will contact meniscal component 26 and act to retard further hyperextension. If hyperextension continues, the area of increased radius of curvature will cause femoral component 22 to lift away from meniscal component 26. The second hyperextension stop mechanism functions at four degrees of hyperextension to prohibit further hyperextension of knee prosthesis 20. The second hyperextension stop mechanism comprises hyperextension stop surface 66 of hinge post 40 and hyperextension stop 68 of bearing box 70. Hyperextension stop surface 66 comprises the concave back wall of cannulated hinge post 40 as illustrated, e.g., in FIGS. 2 and 3. Hyperextension stop 68 of bearing box 70 comprises a protrusion extending from the back wall of bearing box 70 opposite anti-rotation surface 78. Hyperextension stop 68 includes a convex outer surface as illustrated, e.g., in FIG. 12. Hyperextension stop surface 66 of hinge post 40 cooperates with hyperextension stop 68 of bearing box 70 to provide a hyperextension stop for knee prosthesis 20. Concave hyperextension stop surface 66 becomes flush with the convex outer surface of hyperextension stop 68 of bearing box 70 at four degrees of hyperextension to prevent further hyperextension of knee prosthesis 20.

Tibial component 24 is depicted in FIGS. 1-5, 8, 13, and 14. As illustrated, e.g., in FIG. 2, tibial component 24 includes tibial tray 98 connected to tibial stem 92. Stabilizing ribs 94 stabilize tibial tray 98 relative to tibial stem 92 and impede rotation of tibial component 24 in tibia 118 (see, e.g., FIG. 3). In one exemplary embodiment, tibial component 24 is formed from a cobalt-chromium alloy. Tibial component 24 further includes tibial bushing 64 positioned within hinge post extension aperture 110. Tibial bushing 64 is formed of plastic, such as, e.g., UHMWPE and provides a bearing surface between hinge post extension 42 and hinge post extension aperture 110 of tibial component 24. As described above, meniscal component 26 comprises a rotating bearing, and, thus, hinge post extension 42 will rotate relative to tibial component 24. Tibial bushing 64 facilitates this rotation of hinge post extension 42.

Tibial component 24 further includes rotation protrusion 96. As illustrated, e.g., in FIG. 3, rotation protrusion 96 protrudes upwardly from tibial tray 98 of tibial component 24 and further extends in a plane substantially parallel to tibial tray 98. Rotation protrusion 96 cooperates with cutout 90 of meniscal component 26 to guide rotation of meniscal component 26 about hinge post extension 42, as further described hereinbelow.

One embodiment of meniscal component 26 is illustrated in FIGS. 1-7, 13, and 14. Meniscal component 26 is formed from a suitable plastic such as, e.g., UHMWPE and provides a rotating bearing surface between femoral component 22 and tibial component 24. Meniscal component 26 includes bearing surfaces 86, 88 which contact condylar bearing surfaces 28, 30 of femoral component 22 during movement of knee prosthesis 20. As described above, meniscal component 26 further includes hinge post aperture 114 accommodating passage of hinge post 40 and, consequently, hinge post extension 42 therethrough. Meniscal component 26 is operable to rotate about the longitudinal axis of hinge post extension 42 to form a rotating bearing.

Meniscal components of varying heights may be constructed in accordance with the present invention. In one advantageous aspect of the present invention, meniscal component 26 is packaged for sale and use together with hinge

post extension 42 to facilitate component choice and, in one embodiment, to ensure proper extension of hinge post extension 42 into tibial component 24. The extension of hinge post extension 42 into tibial component 24 functions to prevent separation of knee prosthesis 20 after implantation thereof. As is known in the art, the femoral component of a knee prosthesis may, in some situations, move relative to and away from the tibial component in a direction parallel to the longitudinal axis of the hinge post extension. With this in mind, hinge post extension 42 is made to be of sufficient length to be retained within tibial component 24 even in situations in which femoral component 22 moves as described immediately supra. In one exemplary embodiment, hinge post extension 42 extends four centimeters into hinge post extension aperture 110 in tibial component 24.

Meniscal component 26 includes cutout 90 which cooperates with rotation protrusion 96 of tibial component 24 to guide rotation of meniscal component 26 and to resist lifting of meniscal component 26 from tibial tray 98 of tibial component 24. As illustrated, e.g., in FIG. 3, cutout 90 accommodates the portion (i.e., lip) of rotation protrusion 96 extending in a plane substantially parallel to the plane containing tibial tray 98, with a portion (i.e., lip) of meniscal component 26 being positioned between rotation protrusion 96 and tibial tray 98 in a direction substantially perpendicular to the plane containing tibial tray 98. This configuration functions to discourage displacement of meniscal component 26 away from tibial tray 98 in a direction parallel to the longitudinal axis of hinge post extension 42. Furthermore, rotation protrusion 96 acts against the back of cutout 90 to limit rotation of meniscal component 26 about the longitudinal axis of hinge post extension 42.

As illustrated in FIG. 5, meniscal component 26 may be slid out from between tibial component 24 and femoral component 22 when the hinge post extension 42 has been removed from knee prosthesis 20. As illustrated, hinge post aperture 114 is sized to allow rotation of hinge post 40 so that meniscal component 26 may be slid out from its position between femoral component 22 and tibial component 24. This configuration allows for replacement of an implanted meniscal component 26 without requiring removal of hinge post 40. FIG. 5 illustrates removal of hinge post extension 42 to accommodate replacement of meniscal component 26. As illustrated, hinge plug wrench 102 engages hinge plug 38 for removal thereof. After removal of hinge plug 38, slap hammer 104 is threadedly engaged with threaded aperture 44 in hinge post extension 42. Slap hammer 104 may then be utilized to unlock the engagement of locking taper 46 in elongate hinge post extension aperture 112 so that hinge post extension 42 may be removed.

FIGS. 13 and 14 illustrate an alternative embodiment of the knee prosthesis of the current invention. This alternative embodiment utilizes hinge post extension 42a having locking taper 46a, cylindrical extension 48a, and flange 106. In this embodiment, a locking instrument may be utilized to apply force atop hinge post extension 42a so that locking taper 46a is seated in elongate hinge post extension aperture 112 and locked therein. Flange 106 may be utilized to facilitate removal of hinge post extension 42a. As illustrated in FIG. 13, set screw 108 may be utilized as a secondary lock for hinge post extension 42a. In all other respects, the knee prosthesis illustrated in FIGS. 13 and 14 is constructed as described above with respect to the first embodiment of the knee prosthesis in accordance with the present invention.

FIGS. 15, 16 and 17 illustrate an alternative embodiment of the hinge post extension and tibial bushing of the present invention. In this embodiment, tibial component 24a includes

annular tibial bushing expansion groove 122 formed in hinge post extension aperture 110. Tibial bushing 64a includes retaining flange 130 positioned within annular tibial bushing expansion groove 122. FIG. 15 illustrates insertion of cylindrical extension 48b of the hinge post extension into tibial bushing 64a positioned within tibial component 24a. As cylindrical extension 48b proceeds into tibial bushing 64a, bevel 126 contacts annular locking protrusion 128 of tibial bushing 64a and causes outward movement of retaining flange 130 to allow cylindrical extension 48b to proceed to its seated position as illustrated in FIG. 17. Annular tibial bushing expansion groove 122 is sized to allow radial expansion of retaining flange 130 to accommodate placement of cylindrical extension 48b within tibial bushing 64a. In the fully seated position (FIG. 17) cylindrical extension 48b is locked in place by the engagement of annular locking protrusion 128 in annular locking groove 124. Furthermore, retaining flange 130 cooperates with annular tibial bushing expansion groove 122 to prohibit axial displacement of tibial bushing 64a and, consequently, cylindrical extension 48b. In this embodiment, the femoral component is retained in abutting relationship to the meniscal component and lift off of the femoral component is substantially prohibited. Tibial bushing 64a is, in one exemplary embodiment, formed of UHMWPE.

FIGS. 18 and 19 illustrate another alternative embodiment of the knee prosthesis of the current invention. In this embodiment, locking clip 134 is utilized to retain the position of hinge post 40b within hinge post aperture 114 of meniscal component 26a. Hinge post 40b is rotatably attached to femoral component 22 utilizing hinge pin 34 as described above. In this embodiment, hinge post 40b includes locking clip grooves 132, and meniscal component 26a includes locking clip apertures 136. Upon positioning of hinge post 40b within hinge post aperture 114, locking clip 134 is positioned as illustrated in FIG. 19 with each prong of locking clip 134 being inserted into locking clip apertures 136 of meniscal component 26a. As illustrated in FIG. 19, locking clip 134 engages locking clip grooves 132 to retain hinge post 40b within hinge post aperture 114 of meniscal component 26a. In this embodiment, lift off of femoral component 22 is prohibited by the engagement of hinge post 40b with meniscal component 26a. This embodiment of the knee prosthesis of the current invention may further utilize a meniscal component cutout together with a rotation protrusion on the tibial component to resist lifting of the meniscal component from the tibial tray as described above.

FIG. 20 illustrates a further alternative embodiment of the hinge post of the present invention. Hinge post 40c illustrated in FIG. 20 includes reinforcing material 138 to strengthen hinge post 40c.

While this invention has been described as having exemplary designs, the present invention may be further modified within the spirit and scope of this disclosure. This application is therefore intended to cover any variations, uses, or adaptations of the invention using its general principles. Further, this application is intended to cover such departures from the present disclosure as come within known or customary practice in the art to which this invention pertains.

What is claimed is:

- [1. A prosthetic femoral component, comprising:
 - a femoral component body;
 - a hinge post having a longitudinal axis, said hinge post rotatably connected to said femoral component body, said hinge post rotatable relative to said femoral component body about an axis of rotation, said hinge post

9

including an elongate aperture, along said longitudinal axis and elongate aperture transverse to said axis of rotation.]

2. [The prosthetic femoral component of claim 1, further comprising:] *A prosthetic knee assembly, comprising:*
a femoral component body that includes a first internal side wall opposing a second internal side wall;
a hinge pin having a longitudinal hinge pin axis;
a hinge post positioned between the first internal side wall and the second internal side wall of the femoral component body and having a longitudinal hinge post axis, said hinge pin fixed to said femoral component body and passing through a hinge pin aperture in said hinge post for rotatably, hingedly connecting said hinge post to said femoral component body so that rotation of said hinge post relative to said femoral component body is defined about the longitudinal hinge pin axis, said hinge post including an elongate hinge post extension aperture along said longitudinal hinge post axis, said elongate hinge post extension aperture transverse to said longitudinal hinge pin axis; and
 a hinge post extension removeably locked to said hinge post, said elongate hinge post extension aperture of said hinge post sized for placement of said hinge post extension therein, whereby said hinge post extension traverses a first end of said elongate hinge post extension aperture of said hinge post and protrudes from a second end of said elongate hinge post extension aperture of said hinge post.

3. The prosthetic [femoral component] *knee assembly* of claim 2, [further comprising:
 securing means for securing said hinge post extension to said hinge post] *further comprising a tibial component into which the hinge post extension can be received, wherein, when the femoral component is attached to a femur and the tibial component is attached to a tibia opposite the femur, said hinge post extension can be separated from said hinge post to allow rotation of said hinge post about said longitudinal hinge pin axis without having to rotate the femur or tibia about said longitudinal hinge pin axis.*

4. The prosthetic [femoral component] *knee assembly* of claim [3, wherein said securing means comprises:
 a male taper positioned on said hinge post extension; and
 a female taper positioned in said elongate aperture, said male taper engageable in said female taper to secure said hinge post extension to said hinge post] *2 including cooperating locking tapers removeably locking the hinge post extension to the hinge post.*

5. The prosthetic [femoral component] *knee assembly* of claim [1] 2, further comprising:
 a bearing box connected to said femoral component body, said bearing box interposed between said hinge post and said femoral component body, said bearing box including a hyperextension stop, said hinge post including a hyperextension stop surface, said hyperextension stop contacting said hyperextension stop surface to prevent further hyperextension of the [prosthetic] femoral component body beyond a predetermined point of hyperextension.

6. The prosthetic [femoral component] *knee assembly* of claim 5, wherein said predetermined point of hyperextension comprises four degrees of hyperextension of the [prosthetic knee] *femoral component* body.

7. The prosthetic [femoral component] *knee assembly* of claim 5, wherein said hyperextension stop comprises a convex protrusion.

10

8. The prosthetic [femoral component] *knee assembly* of claim 5, wherein said hinge post includes an internal wall, said hyperextension stop surface comprising said internal wall of said hinge post.

[9. A prosthetic femoral component, comprising:
 a femoral component body;
 a hinge post rotatably connected to said femoral component body; and
 a bearing box connected to said femoral component body, said bearing box interposed between said hinge post and said femoral component body, said bearing box including a hyperextension stop, said hinge post including a hyperextension stop surface, said hyperextension stop contacting said hyperextension stop surface to prevent further hyperextension of the prosthetic femoral component body beyond a predetermined point of hyperextension.]

10. [The prosthetic femoral component of claim 9, further comprising:] *A prosthetic knee assembly, comprising:*
a femoral component body;
a hinge post rotatably connected to said femoral component body about a rotational axis;
a bearing box connected to said femoral component body, said bearing box interposed between said hinge post and said femoral component body, said bearing box including a hyperextension stop, said hinge post including a hyperextension stop surface, said hyperextension stop contacting said hyperextension stop surface to prevent further hyperextension of the prosthetic femoral component body beyond a predetermined point of hyperextension; and
 a hinge post extension having a longitudinal axis and being removeably locked to said hinge post, an elongate aperture of said hinge post sized for placement of said hinge post extension therein, whereby said hinge post extension traverses a first end of said elongate aperture of said post and protrudes from a second end of said elongate aperture of said hinge post, wherein the longitudinal axis of said hinge post extension is non-intersecting with said rotational axis.

11. The prosthetic [femoral component] *knee assembly* of claim 10, further comprising:
 securing means for securing said hinge post extension to said hinge post.

12. The prosthetic [femoral component] *knee assembly* of claim 11, wherein said securing means comprises:
 a male taper positioned on said hinge post extension; and
 a female taper positioned in said elongate aperture, said male taper engageable in said female taper to secure said hinge post extension to said hinge post.

13. The prosthetic [femoral component] *knee assembly* of claim [9] 10, wherein said predetermined point of hyperextension comprises four degrees of hyperextension of the [prosthetic] femoral component body.

14. The prosthetic [femoral component] *knee assembly* of claim [9] 10, wherein said hyperextension stop comprises a convex protrusion.

15. The prosthetic [femoral component] *knee assembly* of claim [9] 10, wherein said hinge post includes an internal wall, said hyperextension stop surface comprising said internal wall of said hinge post.

16. A prosthetic knee, comprising:
 a femoral component;
 a tibial component;
 a meniscal component positioned between said femoral component and said tibial component, said femoral component including a condylar bearing surface, said

11

meniscal component including a cooperative bearing surface facing said condylar bearing surface of said femoral component *for contacting said condylar bearing surface*, said femoral component rotatably connected to said tibial component;

a hinge pin having a longitudinal hinge pin axis;

a hinge post rotatably connected to said femoral component *which includes said hinge pin passing through a hinge pin aperture in said hinge post for rotatably, hingedly connecting said hinge post to said femoral component so that rotation of said hinge post relative to said femoral component is defined about the longitudinal hinge pin axis*, said meniscal component including [an] a hinge post aperture with a longitudinal hinge post aperture axis that is non-intersecting with said longitudinal hinge pin axis, said hinge post positioned within said hinge post aperture; and

a locking clip, said meniscal component including a locking clip aperture, said hinge post including a locking clip groove, said locking clip traversing said locking clip aperture and engaging said locking clip groove to retain said hinge post within said hinge post aperture.

[17. A prosthetic knee, comprising:

a femoral component;

a tibial component;

a meniscal component positioned between said femoral component and said tibial component, said femoral component including a condylar bearing surface, said meniscal component including a cooperative bearing surface facing said condylar bearing surface of said femoral component, said femoral component rotatably connected to said tibial component;

a hinge post extension, said hinge post extension rotatably connected to said femoral component, said hinge post extension including an annular groove; and

a tibial bushing including an annular locking protrusion and a retaining flange, said tibial component having a tibial bushing expansion groove, said retaining flange positioned in said tibial bushing expansion groove, said annular locking protrusion engaged in said annular groove.]

12

18. A prosthetic knee, comprising:

a femoral component having a hinge post rotatably connected thereto *about a rotational axis*;

a tibial component;

a meniscal component positioned between said femoral component and said tibial component, said femoral component including a condylar bearing surface, said meniscal component including a cooperative bearing surface facing said condylar bearing surface of said femoral component *for contacting said condylar bearing surface*, said meniscal component including [an] a hinge post aperture having a longitudinal axis that is non-intersecting with said rotational axis, whereby said hinge post is positioned within said hinge post aperture when the prosthetic knee is operably assembled; and

a locking clip, said meniscal component including a locking clip aperture, said hinge post including a locking clip groove, said locking clip traversing said locking clip aperture and engaging said locking clip groove to retain said hinge post within said hinge post aperture.

19. The prosthetic femoral component of claim 2, wherein said first end of said elongate aperture of said hinge post is positioned closer to said hinge pin than said second end of said elongate aperture so that said hinge post extension protrudes from said second end of said elongate aperture of said hinge post in a direction away from said hinge pin.

20. The prosthetic femoral component of claim 10, wherein said first end of said elongate aperture of said hinge post is positioned closer to said femoral component body than said second end of said elongate aperture of said hinge post so that said hinge post extension protrudes from said second end of said elongate aperture of said hinge post in a direction away from said femoral component body.

21. The prosthetic femoral component of claim 2, wherein said hinge pin includes a hexagonal indentation on a first end thereof, said first end being flush with said femoral component, said prosthetic femoral component further comprising a hinge pin plug positioned within said hexagonal indentation and being flush with said first end of said hinge pin.

22. The prosthetic femoral component of claim 2, wherein said longitudinal hinge post axis is non-intersecting with said longitudinal hinge pin axis.

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