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[54] **PHOTOGRAPHING LIGHT QUANTITY CONTROLLER FOR ENDOSCOPE**

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[*] Notice: This patent issued on a continued prosecution application filed under 37 CFR 1.53(d), and is subject to the twenty year patent term provisions of 35 U.S.C. 154(a)(2).

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[21] Appl. No.: **08/763,347**

[22] Filed: **Dec. 11, 1996**

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Related U.S. Patent Documents

Reissue of:

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Filed: **Aug. 21, 1991**

U.S. Applications:

[63] Continuation of application No. 08/395,927, Feb. 28, 1995, abandoned.

Foreign Application Priority Data

Aug. 31, 1990 [JP] Japan 2-231361

[51] **Int. Cl.⁷ G03B 29/00**

[52] **U.S. Cl. 396/17; 396/159; 362/4**

[58] **Field of Search 396/14, 17; 362/4, 362/5, 276; 355/68, 69, 71**

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26 Claims, 14 Drawing Sheets

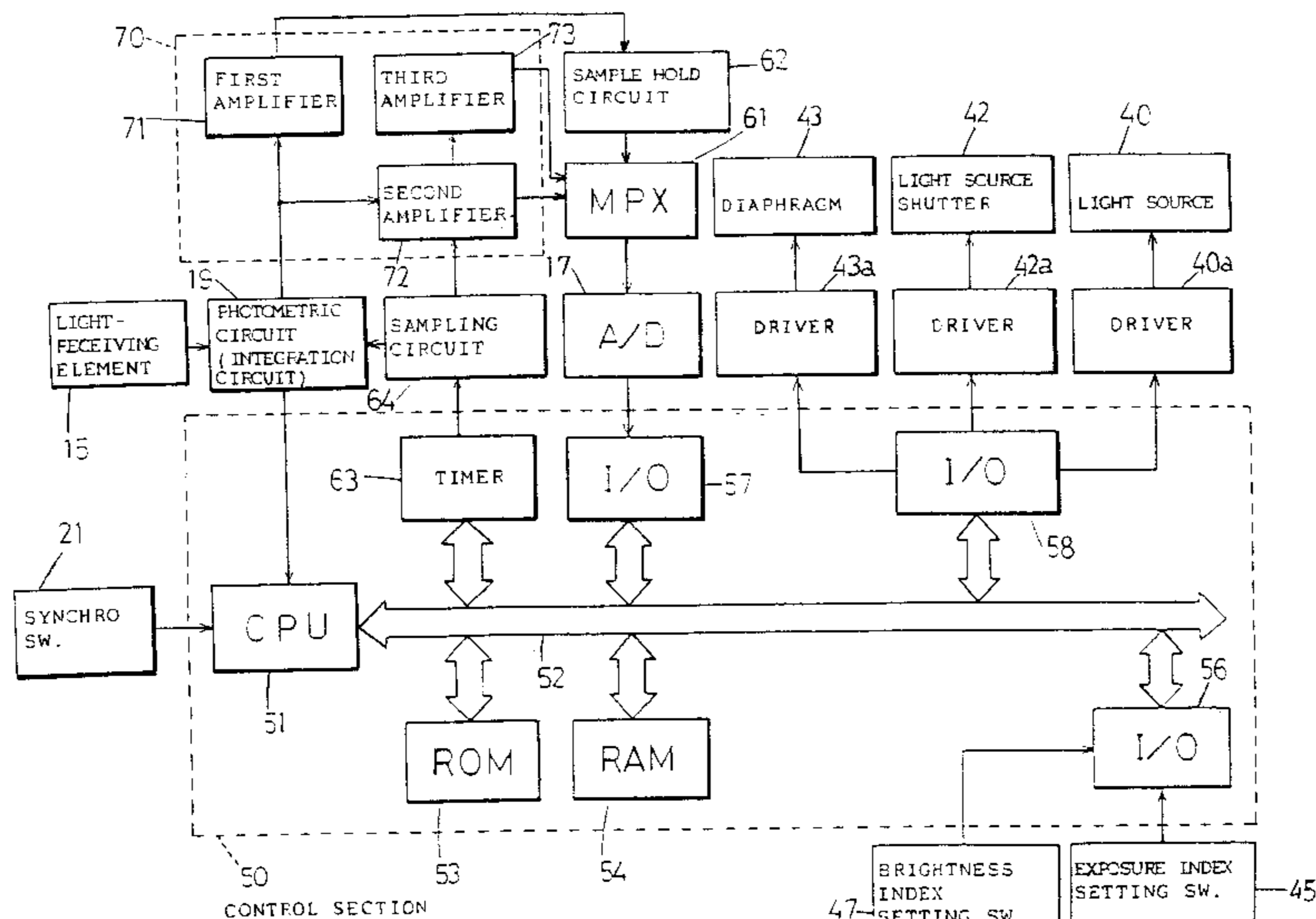


FIG. 1

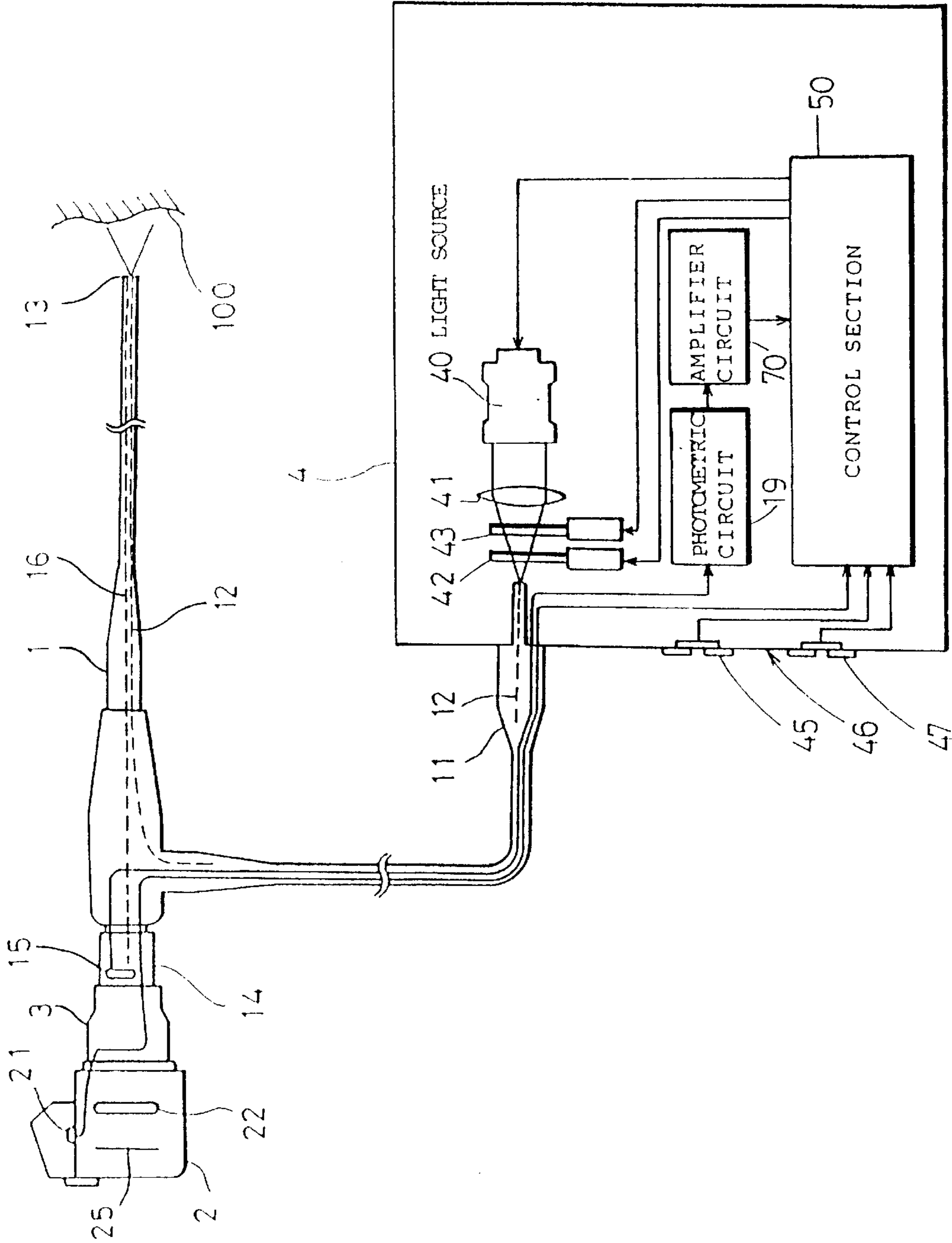


FIG. 2

EXPOSURE IND. EI	0	1	2	3	4	5	6	7	8	9
EXPOSURE QUANTITY (RELATIVE VALUE)	$2^{\frac{5}{2}}$	2^2	$2^{\frac{3}{2}}$	2^1	$2^{\frac{1}{2}}$	1	$2^{\frac{-1}{2}}$	2^{-1}	$2^{\frac{-3}{2}}$	2^{-2}

FIG. 3

BRIGHTNESS INDEX BI	0	1	2	3	4	5	6	7	8	9
BRIGHTNESS (RELATIVE VALUE)	$2^{-\frac{5}{2}}$	2^{-2}	$2^{-\frac{3}{2}}$	2^{-1}	$2^{-\frac{1}{2}}$	1	$2^{\frac{1}{2}}$	2	$2^{\frac{3}{2}}$	2^2

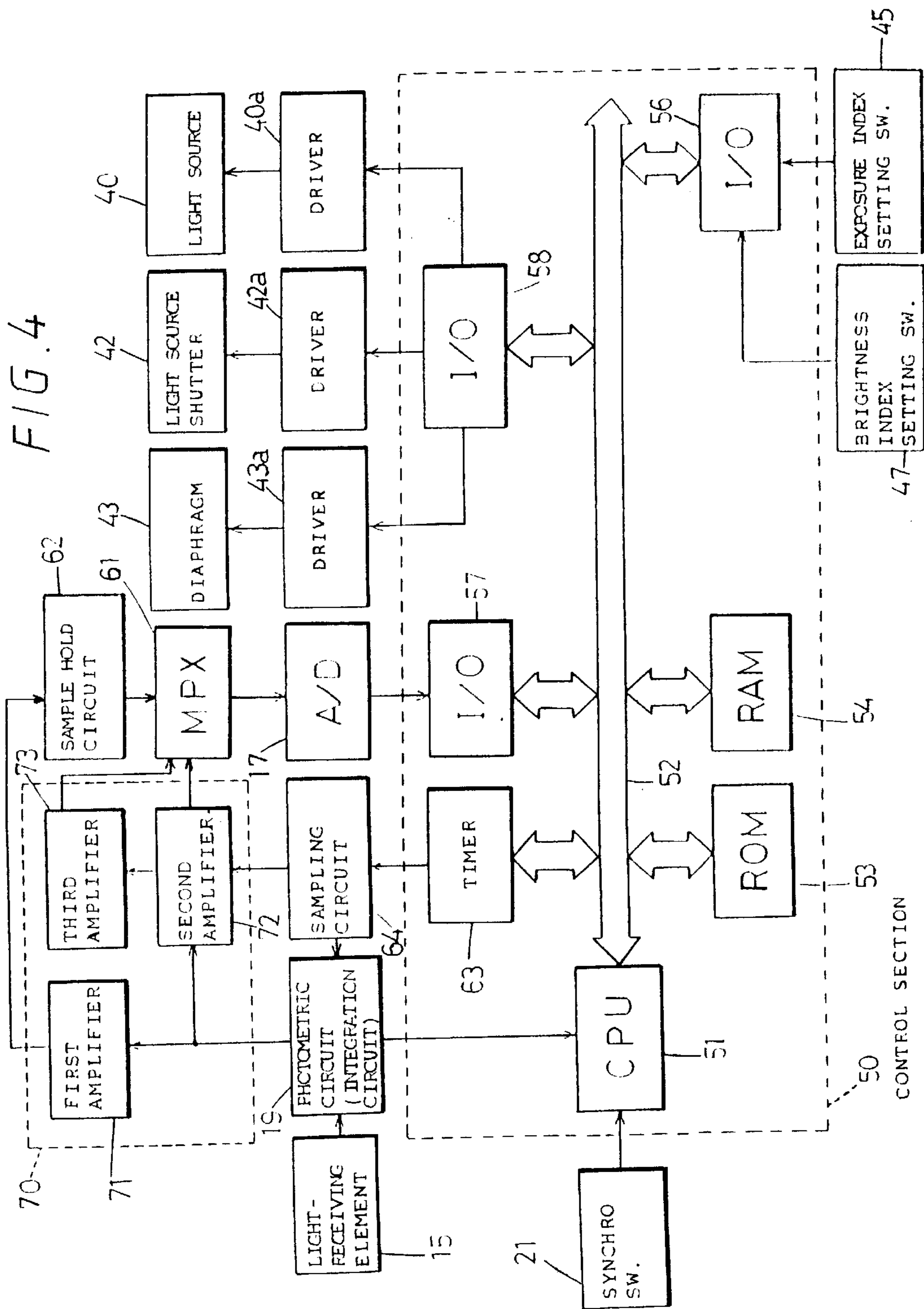


FIG. 5

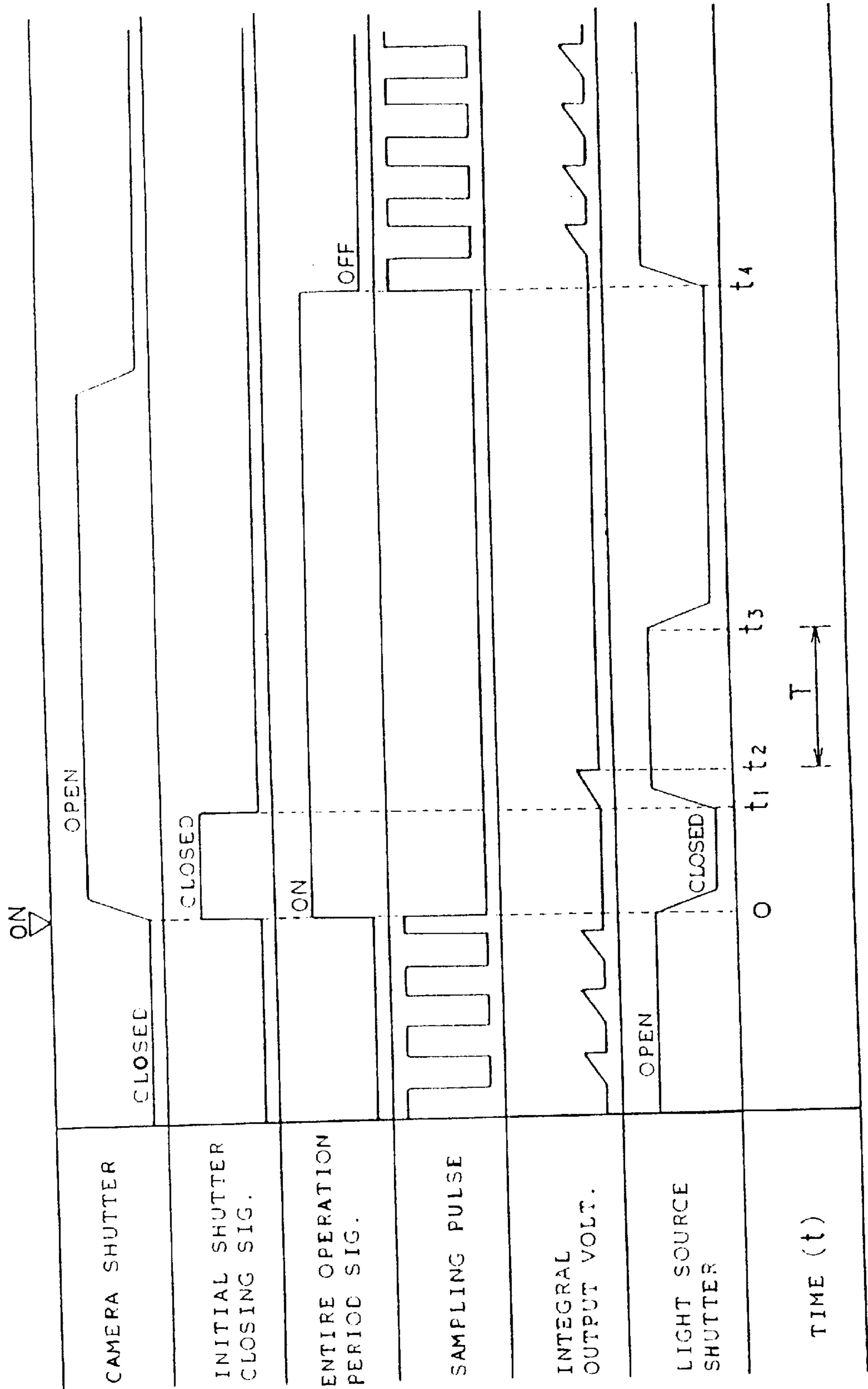


FIG. 6

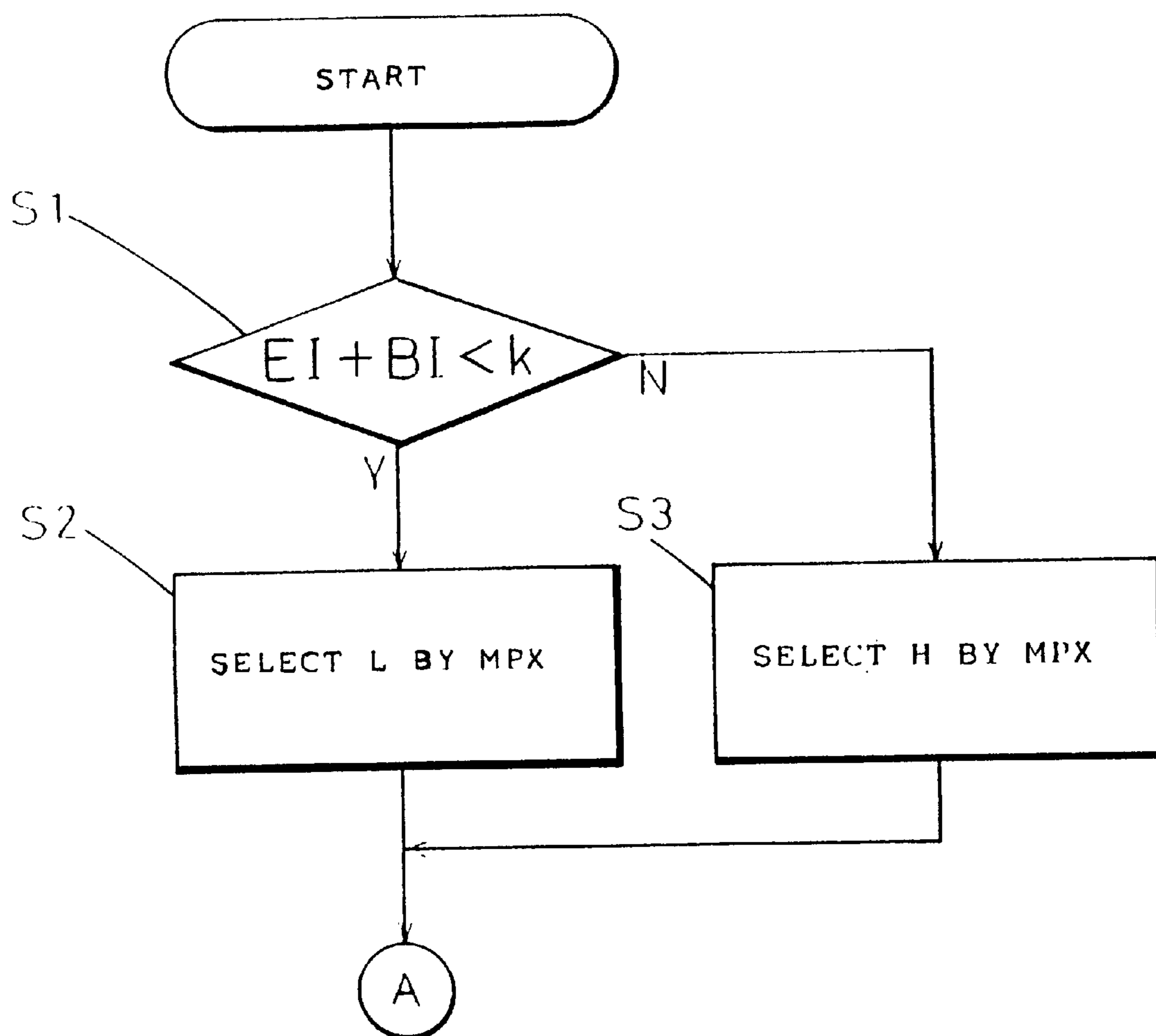


FIG. 7

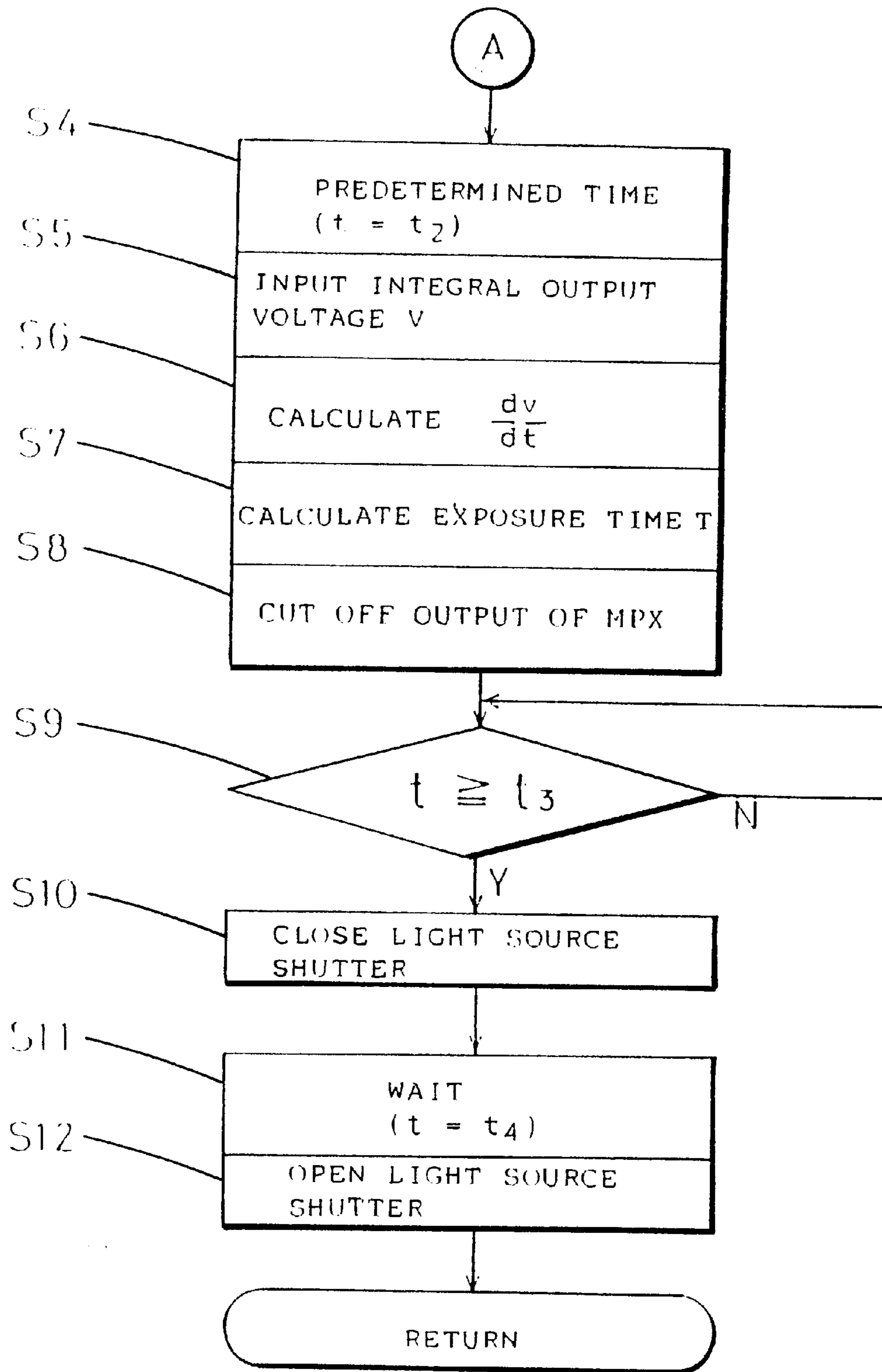


FIG. 8

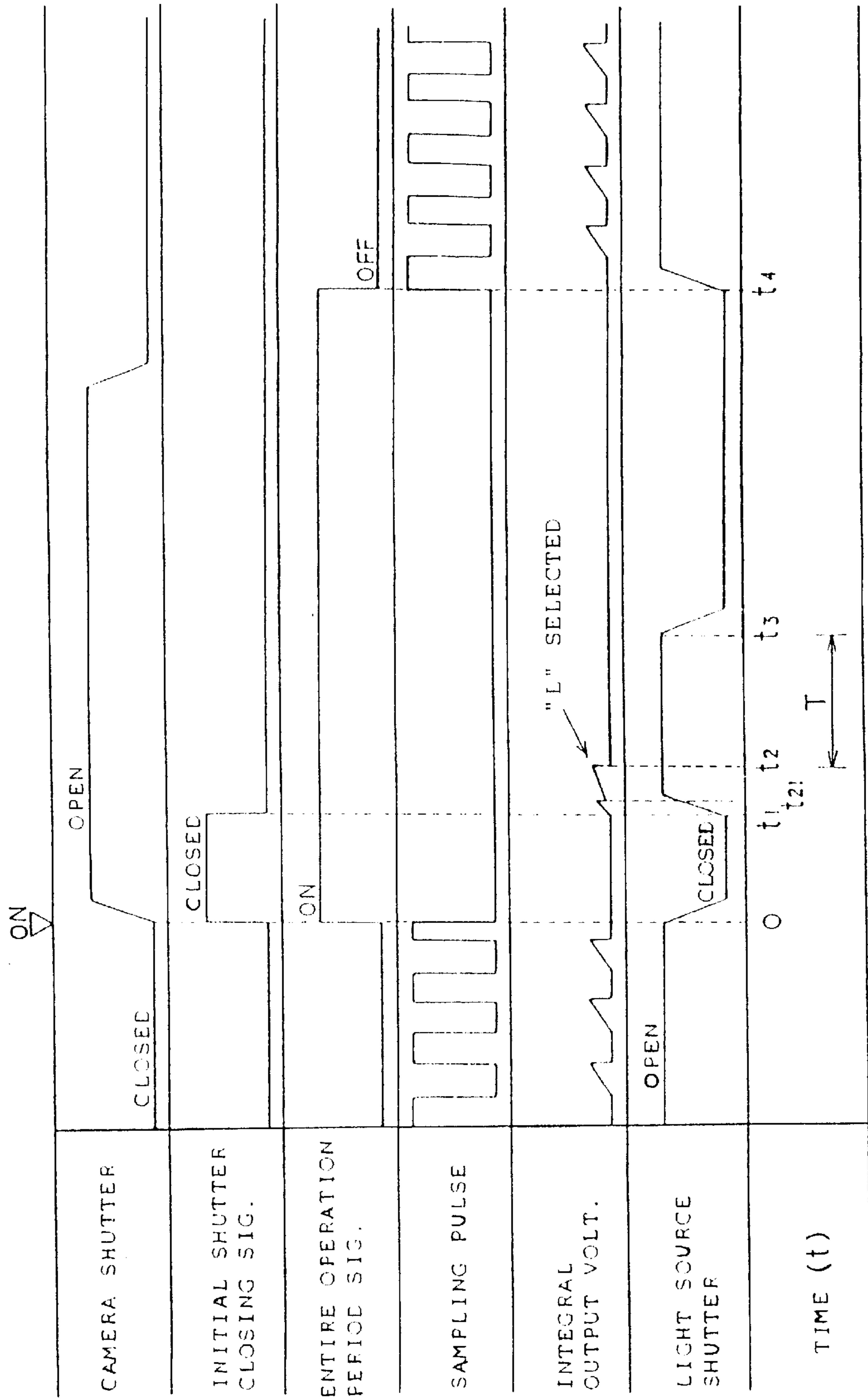


FIG. 9

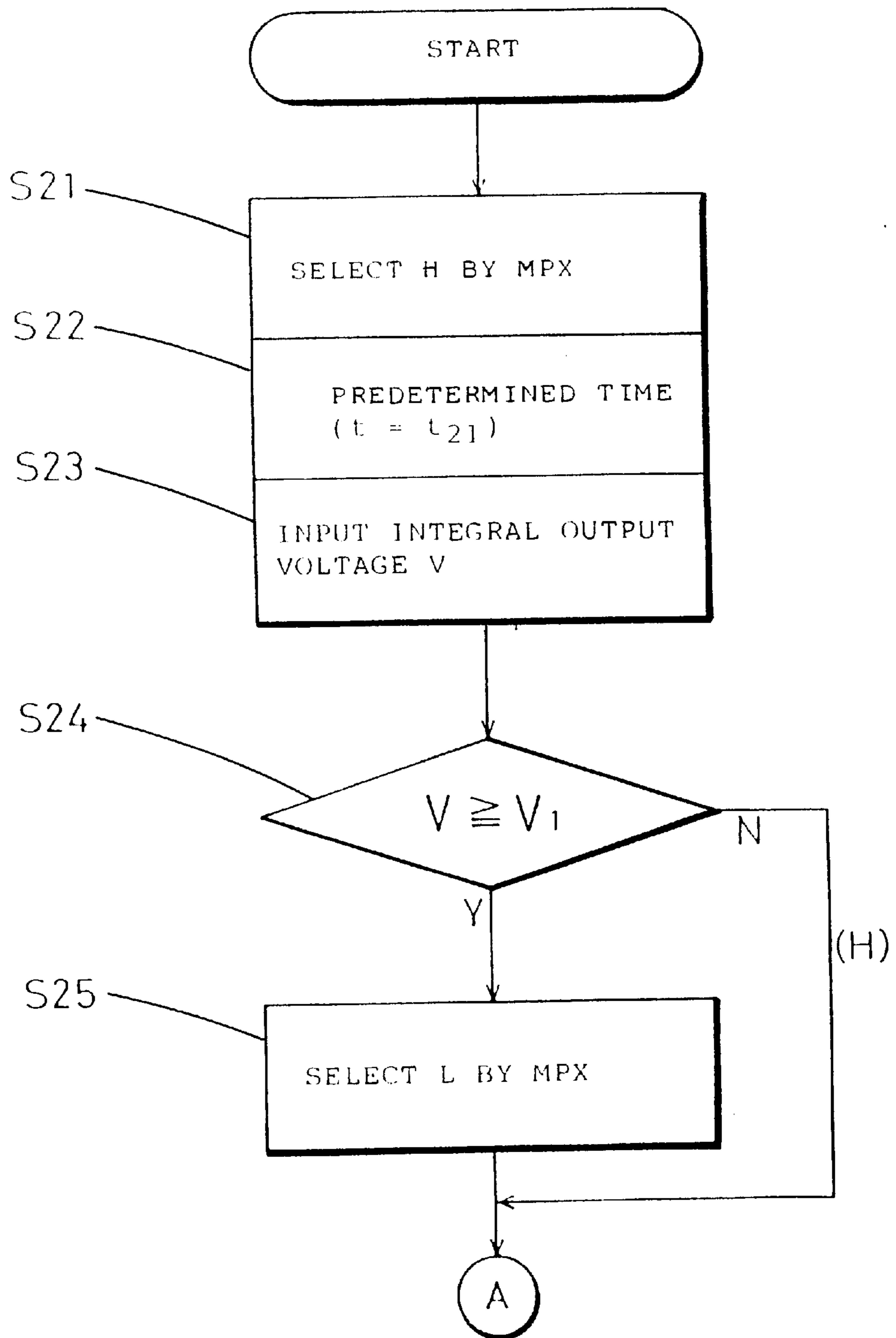


FIG. 10

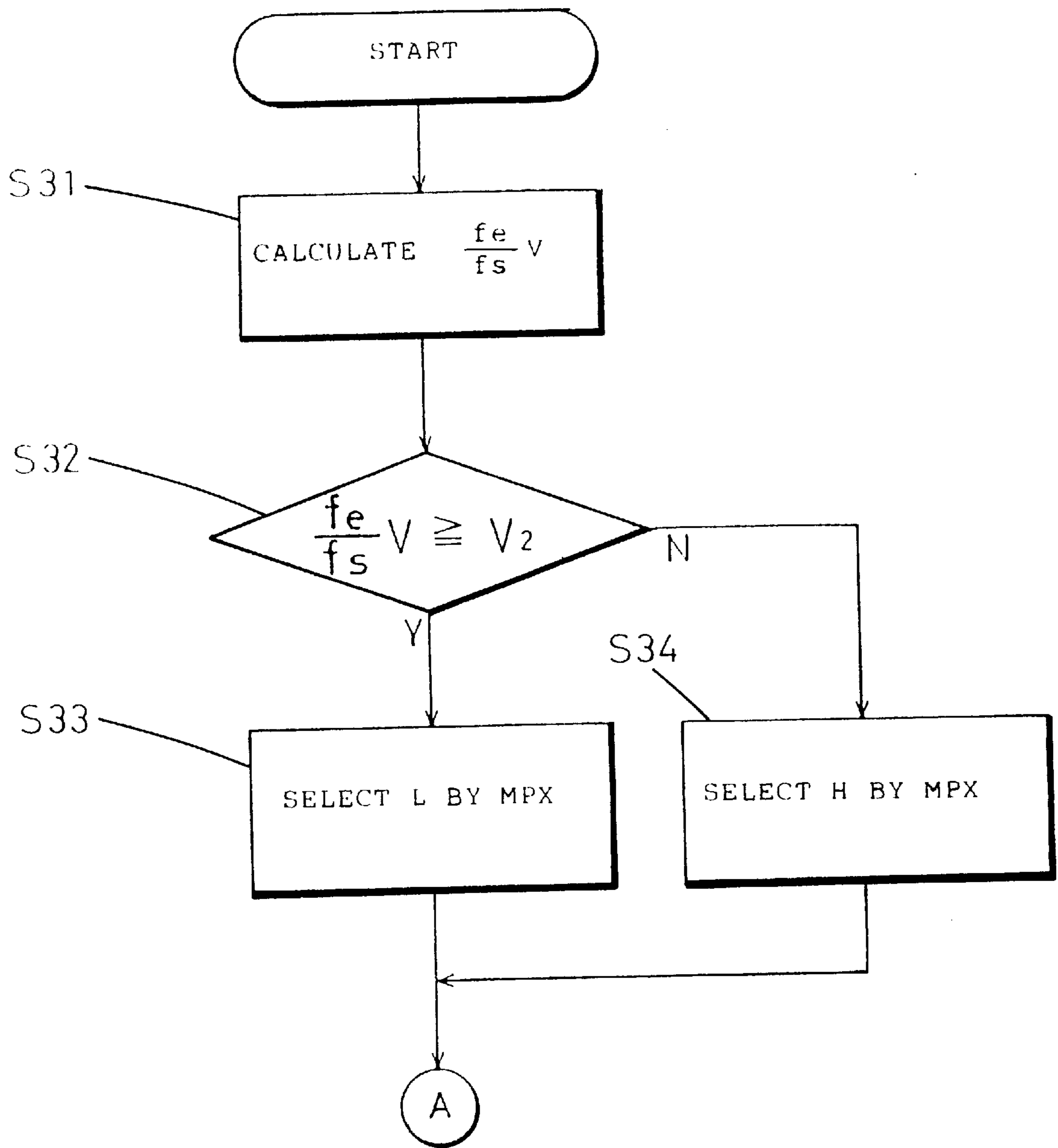


FIG. 11

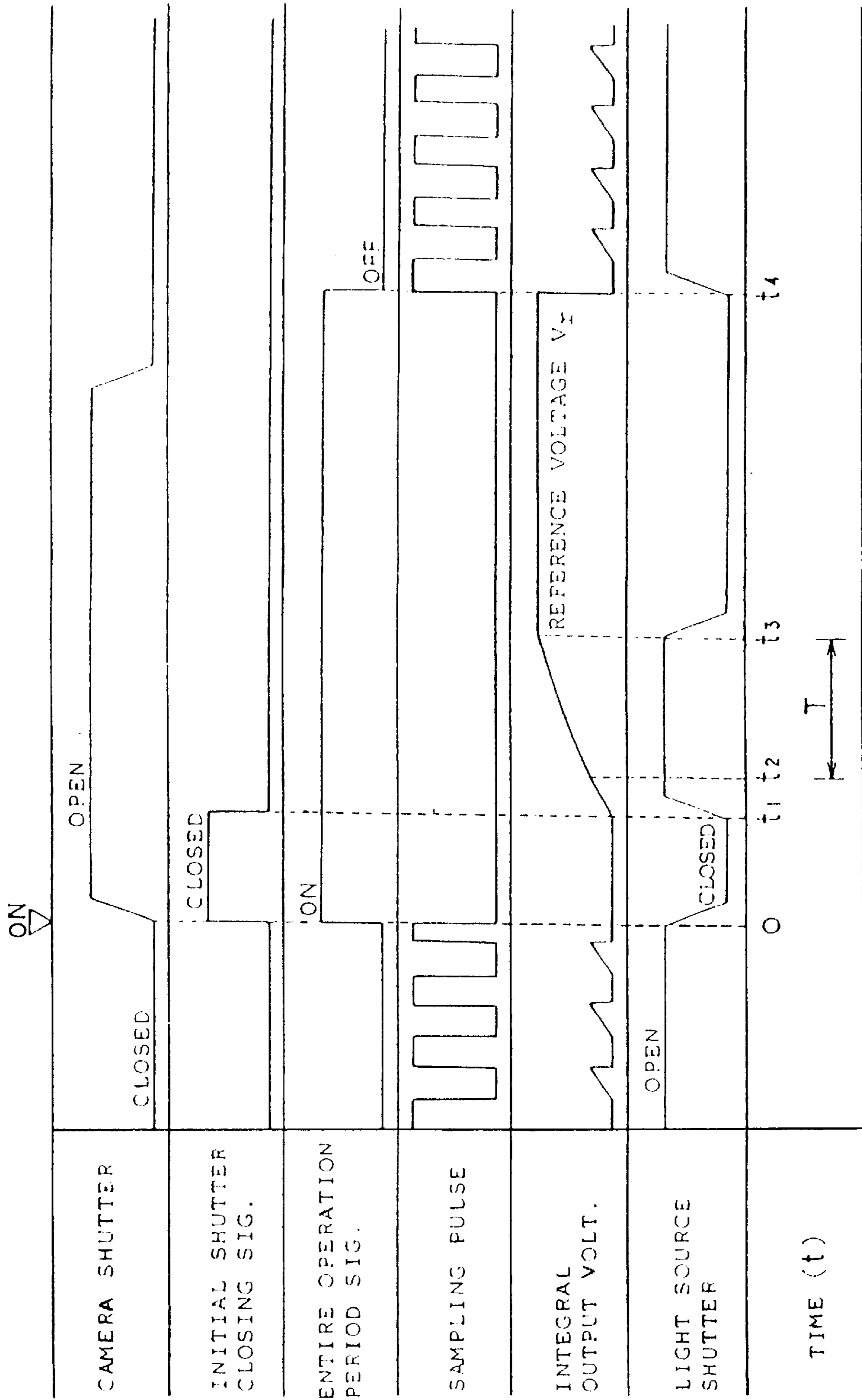


FIG. 12

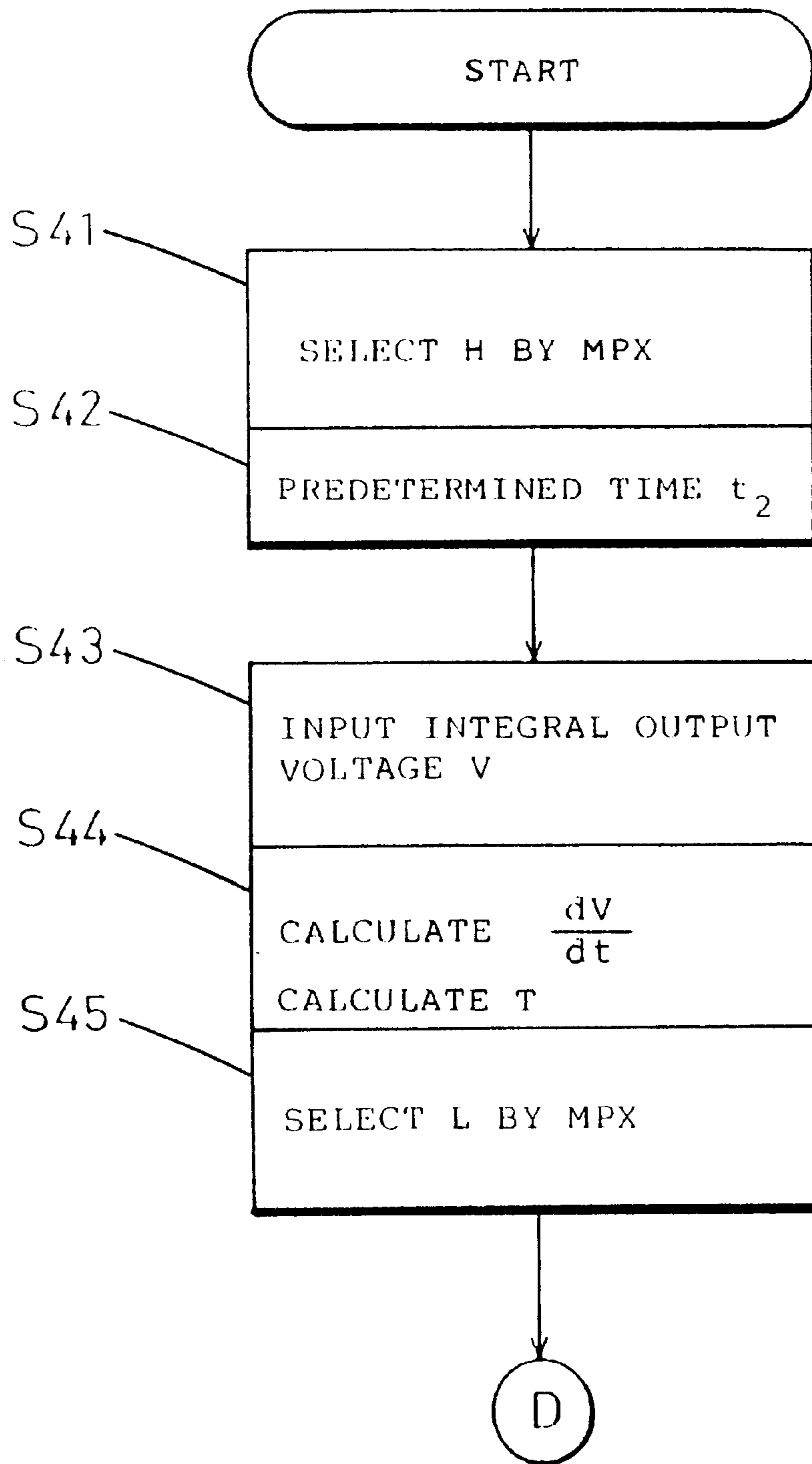


FIG. 13

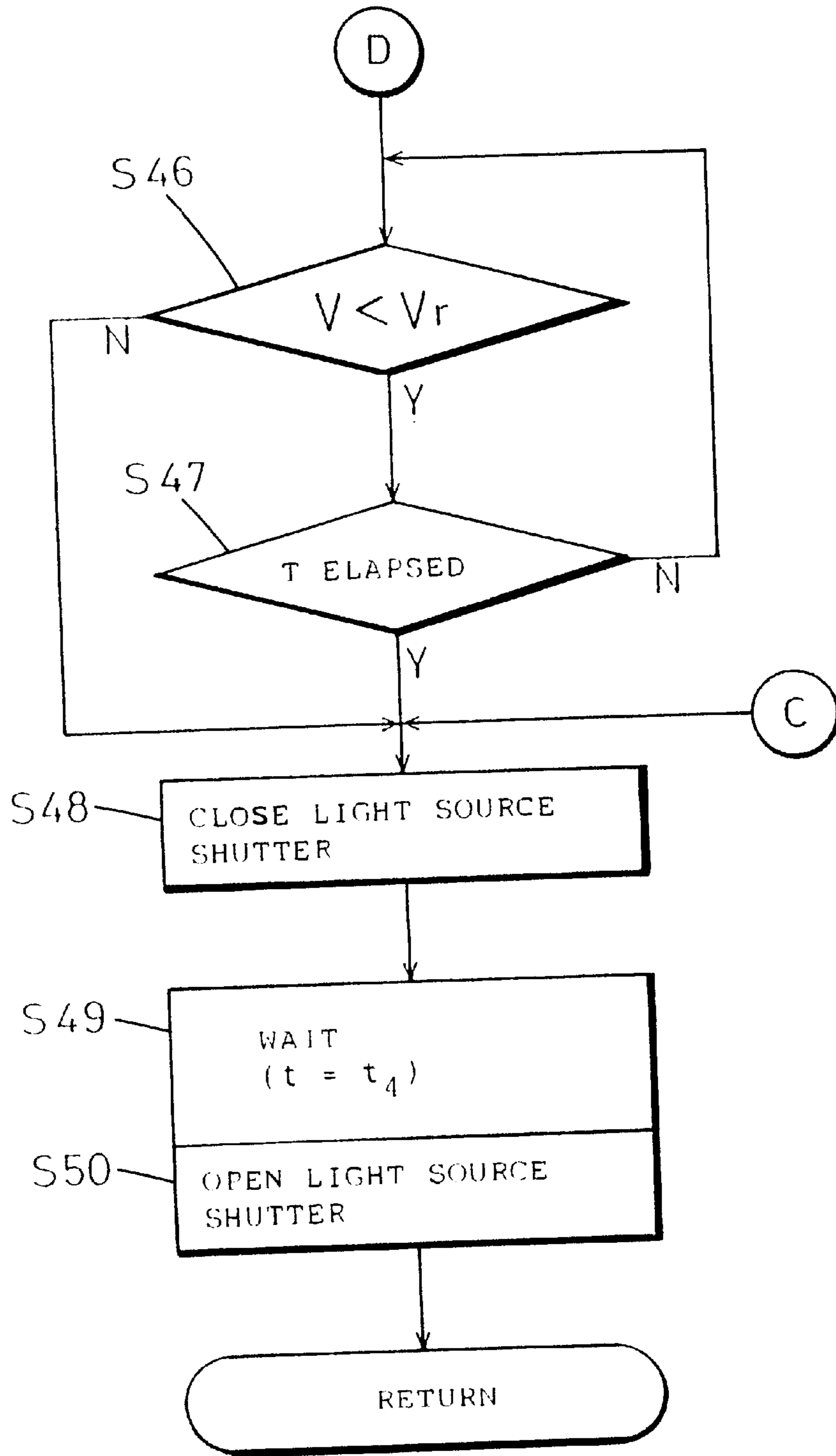
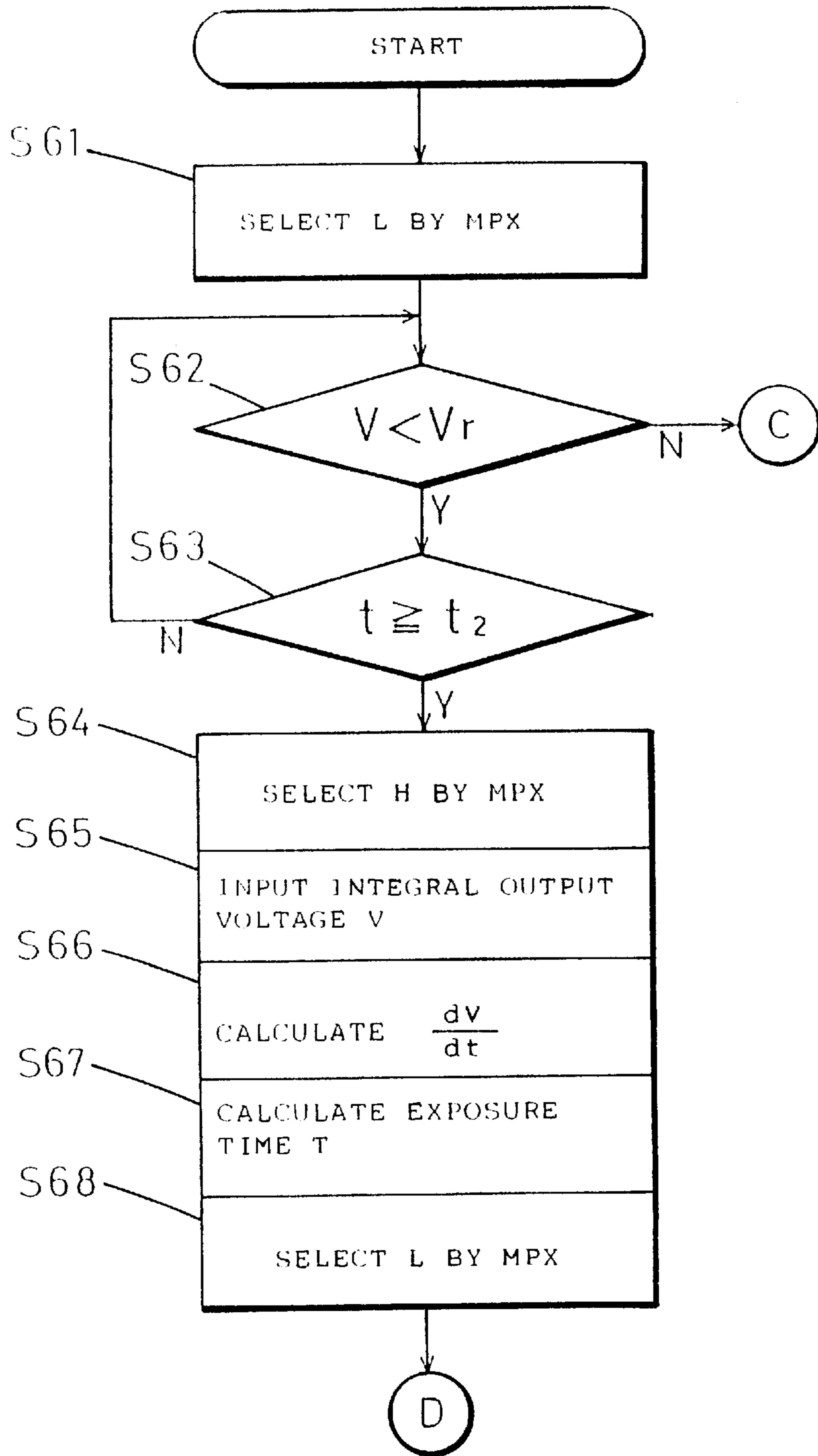


FIG. 14



PHOTOGRAPHING LIGHT QUANTITY CONTROLLER FOR ENDOSCOPE

Matter enclosed in heavy brackets [] appears in the original patent but forms no part of this reissue specification; matter printed in italics indicates the additions made by reissue.

This application is a continuation of application Ser. No. 08/395,927, filed Feb. 28, 1995, now abandoned, which is a Reissue application of U.S. Pat. No. 5,191,369.

BACKGROUND OF THE INVENTION

The present disclosure relates to subject matter contained in Japanese Patent Application No. 2-231361 (filed on Aug. 31, 1990), which is expressly incorporated herein by reference in its entirety.

FIELD OF THE INVENTION

The present invention relates to a photographing light quantity controller for an endoscope, which is used to control the quantity of illuminating light when a photograph is to be taken through the endoscope.

Endoscopes are generally designed to be capable of not only observing the inside of a hollow organ in the patient's body but also taking a photograph of it.

DESCRIPTION OF THE PRIOR ART

In a typical conventional photographing light quantity controller for an endoscope, reflected light from an object, that is illuminated by a light source, is received and converted into an electric signal with a light-receiving element. The output of the light-receiving element is integrated to obtain an integral value. When the integral value reaches a preset reference voltage, the application of the illuminating light to the object is stopped, thus effecting automatic control of the photographing light quantity.

However, since the output signal (voltage) from the light-receiving element is weak, the output voltage is inputted to a photographing light quantity control circuit after being amplified in an amplifier circuit.

A typical conventional amplifier circuit that is employed for this purpose is designed to amplify the input voltage with a fixed amplification factor. Therefore, after a synchro switch is turned on to initiate a photographing operation, the amplifier circuit amplifies the output voltage from the light-receiving element with a constant amplification factor at all times and inputs the amplified voltage to the photographing light quantity control circuit.

Since the object of an endoscope is illuminated with light that is supplied to the endoscope from a light source, the brightness of the object varies in inverse proportion to the square of the distance between the object and the endoscope. Moreover, the object distance range is wide, i.e., from about 5 mm to 10 cm or more, even in a normal use.

Accordingly, when the object is distant and dark, the voltage that is inputted to the photographing light quantity control circuit is considerably low, so that the voltage value may be inaccurate and the signal processing executed in the photographing light quantity control circuit takes a great deal of time. Consequently, the illuminating light quantity control cannot accurately be effected.

In particular, a large error may be produced in a control system wherein an exposure time is predicted from the rate of change of the integral value per unit time (differential with respect to time), immediately after the initiation of an exposure operation.

SUMMARY OF THE INVENTION

An object of the present invention is to provide a photographing light quantity controller for an endoscope, which is capable of accurate, illuminating light quantity control, even when the brightness of the object is remarkably low.

Other objects and advantages of the present invention will become apparent from the following detailed description of illustrated embodiments of the invention.

According to the present invention, there is provided a photographing light quantity controller for an endoscope, which is used to control the quantity of illuminating light when a photograph is to be taken through the endoscope. The photographing light quantity controller comprises a device for supplying light for illuminating an object to the endoscope; a device for photographing the object; a photoelectric conversion device for converting a brightness level of light that is reflected from the object into an electric signal; a device for integrating the output from the photoelectric conversion device and outputting the resulting integral value; a device for amplifying the output value from the integrating device, with the amplifying device having a plurality of amplification factors which can be selected as desired; a photographing light quantity control device for controlling the quantity of illuminating light that is supplied to the endoscope when a photographing operation is conducted, on the basis of the output signal from the amplifying device; a switch for initiating the photographing operation of the photographing device and the control operation of the photographing light quantity control device; and a device for automatically switching over the amplification factors of the amplifying device from one to another in accordance with the brightness of the object.

BRIEF DESCRIPTION OF THE DRAWINGS

The present invention may be more fully understood from the description of the preferred embodiments of the invention set forth below, together with the accompanying drawings, in which:

FIG. 1 is a schematic view showing the whole arrangement of one embodiment of the present invention;

FIG. 2 is a chart showing one example of the setting of exposure indexes;

FIG. 3 is a chart showing one example of the setting of brightness indexes;

FIG. 4 is a circuit block diagram of the embodiment;

FIG. 5 is a time chart showing the operation of the embodiment;

FIGS. 6 and 7 are flowcharts showing a control process in the embodiment;

FIG. 8 is a time chart showing the operation of the second embodiment;

FIG. 9 is a flowchart showing a control process in the second embodiment;

FIG. 10 is a flowchart showing a control process in the third embodiment;

FIG. 11 is a time chart showing the operation of the fourth embodiment;

FIGS. 12 and 13 are flowcharts showing a control process in the fourth embodiment; and

FIG. 14 is a flowchart showing a control process in the fifth embodiment.

DESCRIPTION OF THE EMBODIMENTS

Referring to FIG. 1, which shows the whole arrangement of one embodiment of the present invention, reference

numeral **1** denotes an endoscope. A camera (photographing device) **2** is detachably attached to an eye-piece **14** of the endoscope **1** through a photographic adapter **3**.

Reference numeral **4** denotes a light source apparatus, to which is detachably connected a connector **11** of the endoscope **1**. Illuminating light, that is emitted from a light source (lamp) **40**, is condensed through a condenser lens **41** so as to be made incident on a light guide fiber bundle **12** in the endoscope **1**.

In an illuminating light path, which extends between the light source **40** and the light guide fiber bundle **12**, are provided a shutter (light source shutter) **42** which can be opened and closed to fully open and close the illuminating light path, and a variable diaphragm **43** which is capable of varying the area of passage of the illuminating light.

The illuminating light is transmitted through the light guide fiber bundle **12** and applied to an object **100** from the distal end **13** of an insert part of the endoscope **1**. The reflected light from the object **100** is transmitted through an image guide fiber bundle **16** to expose the plane (photographic plane) of a film **25** in the camera **2**. A shutter **22** in the camera **2** is opened for a predetermined time (e.g., 0.25 sec) only when a synchro switch **21** is turned on.

A light-receiving element **15** is provided in the eye-piece **14** to convert a brightness level of the exposure light that is applied to the plane of the film **25** into an electric signal. The output voltage from the light-receiving element **15** is integrated in a photometric (integration) circuit **19**, and an integral value is outputted from the photometric circuit **19**. The output signal (voltage value) from the photometric circuit **19** is inputted to a control section **50** after being amplified in an amplifier circuit **70**.

The photometric circuit **19** may be provided in either the light source apparatus **4** or the endoscope **1**.

An exposure index setting switch **45** is provided on an operation panel **46** that is attached to the surface of the light source apparatus **4** to set an exposure index **E1** that determines a quantity of light which is to be applied to the photographic plane **25** in the camera **2**. More specifically, the exposure index setting switch **45** is arranged such that the exposure quantity can be controlled in units of 0.5 on the EV exponential valve scale, as shown exemplarily in FIG. 2.

A brightness index setting switch **47** is used to set a brightness level of illuminating light that is supplied to the endoscope **1** when used in an observation state. More specifically, the brightness index setting switch **47** enables the brightness level of illuminating light (i.e., the illuminating light flux that is supplied to the endoscope) during the observation to be controlled by use of the brightness index **BI** set in units of 0.5 on the EV scale, as shown exemplarily in FIG. 3.

Reference numeral **50** denotes a control section which incorporates a microcomputer.

FIG. 4 is a block diagram showing the electrical arrangement of this embodiment. The control section **50** includes a central processing unit (CPU) **51**, and a read only memory (ROM) **53** and a random access memory (RAM) **54**. A system bus **52** connects the CPU **51** to the Rom **53** and the Ram **54**. The CPU **51** is supplied with an interrupt signal which is outputted from the synchro switch **21**.

The system bus **52** is further connected with first to third input/output ports **56**, **57** and **58**. The exposure index setting switch **45** and the brightness index setting switch **47** are connected to the input terminal of the first input/output port **56**.

The output from the light-receiving element **15** is integrated in the photometric (integration) circuit **19** to obtain an integral value (integral output voltage **V**), which is inputted to the amplifier circuit **70**. The amplifier circuit **70** comprises a first amplifier **71**, a second amplifier **72** and a third amplifier **73**, wherein the output from the photometric circuit **19** is inputted to the first and second amplifiers **71** and **72**. The amplified output from the first amplifier **71** is inputted to a multiplexer **61** via a sample-and-hold circuit **62**.

On the other hand, the amplified output from the second amplifier **72** is inputted to the multiplexer **61** through two routes, that is, one that leads the output directly to the multiplexer **61**, and the other that leads the output to the multiplexer **61** via the third amplifier **73** where it is further amplified.

At the time of observation, the peak value of the output signal, that is sampled in the sample-and-hold circuit **62**, is selected in the multiplexer **61**, and the output from the multiplexer **61** is sent to the second input/output port **57** after being converted into a digital signal in an analog-to-digital converter **17**.

At the time of photographing, the output signal from either one of the second and third amplifiers **72** and **73** is selected in the multiplexer **61** and similarly sent to the second input/output port **57** via the analog-to-digital converter **17**.

A clock signal that is outputted from a timer **63** that is connected to the system bus **52** is inputted to a sampling circuit **64**, so that a sampling pulse is outputted from the sampling circuit **64** to the photometric circuit **19** at a predetermined period, in synchronism, with the clock signal. During the observation, when the sampling pulse is at a low level, the photometric circuit **19** performs an integrated operation, whereas, when the sampling pulse is at a high level, the integral output is zero (i.e., $V=0$). The sample frequency is set, for example, at about 500Hz, that is, the integration time is shorter than the exposure time.

The output terminal of the third input/output port **58** is connected to drivers **40a**, **42a** and **43a** which control the brightness of light that is emitted from the light source **40**, the opening and closing operation of the light source shutter **42**, and the degree of opening of the variable diaphragm **43**, respectively.

FIG. 5 is a time chart showing the operation of this embodiment.

When the synchro switch **21** on the camera **2** is turned on, the shutter (camera shutter) **22** in the camera **2** is opened and is closed after a predetermined time (e.g., 0.25 sec) has elapsed. Meantime, the light source shutter **42** in the light source apparatus **4** is temporarily closed at the same time as the synchro switch **21** is turned on. After a predetermined short time (the initial shutter closing time t_1) has elapsed, the light source shutter **42** is opened again in order to emit illuminating light for photographing. The initial shutter closing time t_1 is, for example, 0.035 sec.

Before the synchro switch **21** of the camera **2** is turned on, that is, during the observation, every time the sampling pulse is at the low level, the output voltage from the light-receiving element **15** is integrated, and the peak value of the integral output voltage that is passed through the first amplifier **71** and the sample-and-hold circuit **62** is selected in the multiplexer **61** and inputted to the CPU **51**.

After the light source shutter **42** has been opened, to expose the film plane **25**, and the time t_2 has elapsed since the turning on of the synchro switch **21**, the rate of change

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of the integral output voltage V per unit time (i.e., differential with respect to time) dV/dt so far is obtained. Assuming that ΔV is the integral output voltage V at the time t_2 ,

$$dV/dt=(1/a) \cdot C \cdot \Delta V / (t_2 - t_1)$$

where a is an amplification factor in the amplifier circuit **70**, and C is a correction coefficient.

The predicted exposure time T , remaining after t_2 has elapsed, is obtained as follows:

$$T=(V_r - \Delta V/a) \cdot dt/dV$$

where V_r a reference voltage.

Before the remaining predicted exposure time T is obtained in this way, it is determined which of the output signals from the second and third amplifiers **72** and **73** is to be employed for the calculation.

The reason for this is to avoid the problem that values which are obtained by calculating dV/dt , according to the above equation, involve large errors and are therefore unreliable unless ΔV is greater than a certain value and the problem that, if ΔV is excessively large, the load that is applied to electronic elements, such as the analog-to-digital converter **17**, exceeds the maximum input ratings, causing destruction of the electronic elements.

More specifically, when the exposure index EI is large (i.e., when the reference voltage V_r is low), it is preferable to lower the brightness level of the illuminating light. In such a case, dV/dt must be calculated with a small integral output voltage V . At this time, therefore, the output (hereinafter referred to as "H") from the third amplifier **73** is selected in the multiplexer **61** in order to increase the amplification factor. When the brightness index BI is large (i.e., when the brightness level of the illuminating light supplied to the endoscope **1** from the light source apparatus **4** during the observation is high), the object **100** is considered to be distant and rather dark. Therefore, at this time also, the output H from the third amplifier **73** is selected in the multiplexer **61**.

Thus, it is possible to obtain precise dV/dt within a short period of time and effect accurate exposure control.

In cases contrary to the above, the output (hereinafter referred to as "L") from the second amplifier **72**, with a relatively low amplification factor, is selected.

When numerical values such as those shown in FIGS. **2** and **3** are employed, the above-described selection judgment may be made by setting k in the following equations at $k=15$, for example:

When $EI+BI \geq k$, H is selected; and

When $EI+BI < k$, L is selected.

For H , the amplification factor is, for example, from **3** to **4**, and for L , for example, from **1** to **2**.

After dV/dt is obtained, the output to the analog-to-digital converter **17** is cut off by the multiplexer **61**. The reason for this is to prevent the analog-to-digital converter **17** from being fed with a voltage that exceeds the maximum input rating thereof.

When the predicted exposure time T has elapsed, the light source shutter **42** is closed again. When the entire operation terminating time t_4 (e.g., 0.5 sec) has elapsed since the turning on of the synchro switch **21**, all the elements of the system return to the previous state, i.e., the state before the turning on of the synchro switch **21**. Thus, the light source shutter **42** opens again to provide an observation state.

FIGS. **6** and **7** are flowcharts showing a process that is executed by software stored in the ROM **53** to effect the above-described control operation. In the figures, S denotes Steps.

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This process is initiated when the synchro switch **21** is turned on. First, $EI+BI$ is compared with a predetermined value k at **S1**. When $EI+BI$ is smaller than k , the output L from the second amplifier **72** is selected in the multiplexer **61** at **S2**. When $EI+BI$ is not smaller than k , the output H from the third amplifier **73** is selected in the multiplexer **61** at **S3**.

In this way, the amplification factor that is employed in the amplifier circuit **70** is automatically switched over from one to another after the synchro switch **21** is turned on.

Next, the elapse of a predetermined value t_2 is awaited at **S4**, the integral output voltage V is inputted at **S5**, and dV/dt is calculated at **S6**.

Then, the remaining predicted exposure time T is calculated on the basis of the value of dV/dt at **S7**, and the output of the multiplexer **61** is cut off at **S8**.

Next, when it is detected at **S9** that the predicted exposure time T has reached the time t_3 , the light source shutter **42** closed at **S10**. Then, the elapse of the entire operation terminating time t_4 is awaited at **S11**, and the light source shutter **42** is opened again at **S12** to return to the previous observation state.

It should be noted that the way of switching the amplifier circuit in the present invention is not necessarily limited to the foregoing embodiment and that it may be carried out in various other forms.

Other forms of switching the amplifier circuit in the present invention will be explained below. In the following, description of portions or elements that perform the same operations as in the above-described embodiments is omitted.

FIG. **8** shows an arrangement in which the integral output voltage V is inputted immediately after the light source shutter **42** is opened (e.g., from 0.001 to 0.002 sec after it), i.e., at t_{21} , and either the output L from the second amplifier **72** or the output H from the third amplifier **73** is selected in accordance with the input value.

However, the integral output voltage V at t_{21} is not employed for calculation of dV/dt . This is because the integral output voltage V , at this point of time is very small and hence influenced greatly by the noise or by the fluctuation of the motion of the light source shutter **42**.

Accordingly, the calculation of dV/dt is performed when the time t_2 has elapsed since the turning on of the synchro switch **21**, and the remaining exposure time T is calculated at that time.

FIG. **9** is a flowchart showing a process for executing the above-described operation. In this case, when the synchro switch **21** is turned on, the output H from the third amplifier **73** is first selected in the multiplexer **61** at **S21**. Next, after a predetermined time t_{21} has elapsed at **S22**, the integral output voltage V is inputted at **S23**.

Then, if the integral output voltage V is equal to or greater than a reference value V_1 at **S24**, the output L from the second amplifier **72** is selected in the multiplexer **61** at **S25**, whereas, if the integral output voltage V is smaller than the reference value V_1 at **S24**, the output H from the third amplifier **73** is left in the selected state. Thereafter, the process proceeds to **S4** in FIG. **7**.

FIG. **10** is a flowchart showing a control process wherein the selection of an amplifier is effected on the basis of the integral output voltage V that is obtained in response to the sampling pulse during the normal observation. In this case, when the synchro switch **21** is turned on, $V \cdot fe/fs$ is calculated at **S31**. In the expression, fe is the aperture of the diaphragm **43** during photographing, and fs is the aperture of the diaphragm **43** immediately before photographing is initiated.

Next, if $V \cdot fe/fs$ is equal to or greater than a reference value V_2 at S32, the output L from the second amplifier 72 is selected in the multiplexer 61 at S33. Conversely, if $V \cdot fe/fs$ is smaller than the reference value V_2 at S32, the output H from the third amplifier 73 is selected in the multiplexer 61 at S34. Thereafter, the process proceeds to S4 in FIG. 7.

In the foregoing embodiments, dV/dt is obtained to calculate the remaining predicted exposure time T, and when the exposure time T has elapsed, the light source shutter 42 is closed.

In the following embodiment, the integral output voltage V is constantly monitored after the light source shutter 42 is opened, and when the voltage value reaches a reference voltage V_r . Also the light source shutter 42 is closed to terminate the exposure operation, as shown in FIG. 11, thereby effecting even more careful control.

In this case, when dV/dt is obtained after the time t_2 has elapsed since the turning on of the synchro switch 21, the output H from the third amplifier 73 is selected, thereby accurately obtaining dV/dt within a short period of time. Thereafter, the output L from the second amplifier 72 is selected to prevent breakage of the electronic elements due to an excess voltage.

It should be noted that the time t_2 in the above-described embodiments need not be coincident with each other.

FIGS. 12 and 13 are flowcharts showing the above-described control process.

When the synchro switch 21 is turned on, the output H from the third amplifier 73 is selected in the multiplexer 61 at S41, and then the elapse of the time t_2 is awaited at S42.

When the time t_2 has elapsed, the integral output voltage V is inputted at S43, and dV/dt and T are calculated at S44. Then, the output L from the second amplifier 72 is selected at S45.

When the integral output voltage V reaches a reference voltage V_r at S46 or the predicted exposure time T has elapsed at S47, the light source shutter 42 is closed at S48.

Next, the elapse of the entire operation terminating time t_4 is awaited at S49, and the light source shutter 42 is then opened at S50 to return to the normal observation state.

FIG. 14 is a flowchart showing a control process that takes into consideration a case where the integral output voltage V reaches the reference voltage V_r before the elapse of the time t_2 for obtaining dV/dt .

In this process, when the synchro switch 21 is turned on, the output L from the second amplifier 72 is selected in the multiplexer 61 at S61. If it is decided at S62 and S63 that the integral output voltage V reaches the reference voltage V_r before the time t_2 has elapsed, the process proceeds to S48 in FIG. 13 to close the light source shutter 42.

If it is decided at S62 and S63 that the integral output voltage V has not yet reached the reference voltage V_r when the time t_2 has elapsed, the output H from the third amplifier 73 is selected in the multiplexer 61 at S64, and the integral output voltage V is inputted at S65.

Then, dV/dt is calculated at S66, the remaining predicted exposure time T is calculated at S67, and the output L from the second amplifier 72 is selected in the multiplexer 61 at S68. Thereafter, the process proceeds to S46 in the FIG. 13.

Although the foregoing embodiments employ two different kinds of amplifier which are selected after the synchro switch 21 is turned on, it should be noted that the number of such amplifiers may be increased to effect even more delicate control.

In addition, the amplification factor H need not be fixed. For example, H may be selected from among a plurality of amplification factors in a similar manner to that in the embodiments shown in FIGS. 1 to 11.

According to the present invention, the amplification factor for the integral output voltage is automatically switched over from one to another in accordance with the brightness of the object. Accordingly, it is possible to obtain a signal with a proper level independently of the brightness of the object and hence possible to effect accurate photographing light quantity control. Thus, photographing of high quality can be performed.

While the invention has been described by reference to specific embodiments chosen for purposes of illustration, it should be apparent that numerous modifications could be made thereto by those skilled in the art without departing from the basic concept and scope of the invention.

We claim:

1. A photographing light quantity controller for an endoscope, which is used to control a quantity of illuminating light when a photograph is to be taken through said endoscope, comprising:

means for supplying light for illuminating an object to said endoscope;

means for detecting a quantity of light that is reflected from said object and for outputting a signal in accordance with the detected quantity of light;

means for amplifying said signal, said amplifying means having a plurality of amplification factors which can be selected as desired;

photographing light [quality] quantity control means for controlling the quantity of illuminating light that is supplied to said endoscope when a photographing operation is conducted, on a basis of the output signal from said amplifying means; and

means for automatically switching over said amplification factors of said amplifying means from one to another in accordance with a brightness of said object.

2. A photographing light quantity controller for an endoscope, which is used to control a quantity of illuminating light when a photograph is to be taken through said endoscope, comprising:

means for supplying light for illuminating an object to said endoscope;

a device for photographing said object;

photoelectric conversion means for converting a brightness level of light, that is reflected from said object, into an electric signal;

means for integrating an output from said photoelectric conversion means and outputting a resulting integral value;

means for amplifying the output value from said integrating means, said amplifying means having a plurality of amplification factors which can be selected as desired;

photographing light quality control means for controlling the quantity of illuminating light that is supplied to said endoscope when a photographing operation is conducted, on a basis of the output signal from said amplifying means;

a switch for initiating said photographing operation of said photographing device and said control operation of said photographing light quantity control means; and

means for automatically switching over said amplification factors of said amplifying means from one to another in accordance with a brightness of said object.

3. A photographing light quantity controller for an endoscope according to claim 2, wherein said amplifying means has a plurality of amplifiers with different amplification factors.

4. A photographing light quantity controller for an endoscope according to claim 2, wherein said amplification factors are switched over in such a manner that, when the output value from said integrating means is small, an amplification factor switching means selects a large amplification factor from among said plurality of amplification factors of said amplifying means, whereas, when the output value from said integrating means is large, said amplification factor switching means selects a small amplification factor from among said plurality of amplification factors.

5. A photographing light quantity controller for an endoscope according to claim 4, wherein said amplification factors switching means switches over said amplification factors from one to another after said switch is turned on.

6. A photographing light quantity controller for an endoscope according to claim 4, wherein said amplification factor switching means switches over said amplification factors from one to another before said switch is turned on.

7. A photographing light quantity controller for an endoscope according to claim 2, wherein said integrating means integrates the output from said photoelectric conversion means for a period of time which is shorter than an exposure time immediately after exposure has been initiated, at least with respect to a photographing plane in said photographing device.

8. A photographing light quantity controller for an endoscope according to claim 2, wherein said photographing light quantity control means obtains a rate of change of the output value from said amplifying means per unit time and controls the quantity of illuminating light for photographing on a basis of the value obtained.

9. A photographing light quantity controller for an endoscope according to claim 8, wherein said photographing light quantity control means calculates remaining exposure time required to obtain the quantity of illuminating light for photographing from said rate of change of the output value from said amplifying means per unit time and terminates the supply of the illuminating light to said endoscope after said remaining exposure time has elapsed.

10. A photographing light quantity controller for an endoscope according to claim 8, wherein said photographing light quantity control means terminates the supply of the illuminating light to said endoscope when the output value from said amplifying means reaches a predetermined value.

11. A photographing light quantity controller for an endoscope according to claim 5, wherein said amplification factor switching means selects one said amplification factors on the basis of the output value from said amplifying means that is delivered a short time after said switch is turned on.

12. A photographing light quantity controller for an endoscope according to claim 11, wherein said photographing light quantity control means controls the quantity of illuminating light for photographing on a basis of a rate of change of the output value from said amplifying means per unit time after an amplification factor is selected by said amplification factor switching means.

13. A photographing light quantity controller for an endoscope according to claim 12, wherein said amplification factor of said amplifying means, this is employed when said photographing light quantity control means controls the quantity of illuminating light, is not larger than said amplification factor of said amplifying means that is employed when said amplification factor switching means selects said amplification factor.

14. A photographing light quantity controller for an endoscope according to claim 2, further comprising means for making a comparison between the integral value, outputted

from said integrating means after said switch has been turned on, and a preset reference value, and for terminating the supply of the illuminating light to said endoscope when said integral value reaches said reference value.

15. A method for controlling a quantity of photographing light for an endoscope when a photograph of an object is taken through said endoscope during a photographing operation, the method comprising:

supplying light for the illumination of said object to said endoscope by an illuminating device;

detecting a quantity of light reflected by said object;

generating a light quantity signal corresponding to said quantity of light;

integrating said light quantity signal and emitting a resultant integral value;

controlling said quantity of photographing light which is supplied to said endoscope when carrying out a photographing operation depending on said integral value;

calculating, after a first period of time after the beginning of exposure, a remaining exposure time from said resultant integral value in the photographing operation; and

amplifying said resultant integral value by a first amplification factor during said first time period, and a second amplification factor during the remaining exposure time after calculation of the remaining exposure time.

16. The method according to claim 15, wherein said first amplification factor is higher than said second amplification factor.

17. The method according to claim 15, further comprising amplifying said resultant integral value by a third amplification factor before said first period of time, said third amplification factor being lower than said first amplification factor.

18. The method of claim 15, comprising converting a brightness level of said light reflected by said object into an electric signal and calculating said remaining exposure time for reaching the required quantity of photographing light from an increase of the resultant integral value amplified per unit time.

19. The method according to claim 15, further comprising:

comparing said resultant integral value with a reference value during the duration of exposure; and

stopping said exposure upon a first occurrence of one of said remaining exposure time elapsing and said resultant integral value reaching said reference value.

20. A photographing light quantity controller for an endoscope which is used to control a quantity of illuminating light when a photograph is to be taken through said endoscope, comprising:

means for supplying light for illuminating an object to said endoscope;

means for detecting a quantity of light that is reflected from said object and for outputting a signal in accordance with the detected quantity of light;

a device for integrating said light quantity signal outputted by said detecting means and for emitting a resulting integral value, said resultant integral value being an integral output voltage;

photographing light quantity control means for controlling the quantity of illuminating light that is supplied to said endoscope when a photographing operation is conducted, depending on said resultant integral value;

a device for calculating a remaining exposure time from said resultant integral value after a first period of time after a beginning of exposure in the photographing operation; and

an amplifying system that amplifies said resultant integral value by a first amplification factor during said first time period, and by a second amplification factor during the remaining exposure time after calculation of the remaining exposure time.

21. *A photographing light quantity controller for an endoscope according to claim 15, wherein said amplifying system is operable using a plurality of amplification factors, and including a device that automatically switches over said plurality of amplification factors of said amplifying system so that said resultant integral value is amplified by said first amplification factor during said first period of time and by said second amplification factor during said remaining exposure time after calculation of said remaining exposure time.*

22. *A photographing light quantity controller for an endoscope according to claim 20, wherein said amplifying system comprises a plurality of amplifiers having different amplification factors.*

23. *A photographing light quantity controller for an endoscope according to claim 20, wherein said means for detecting comprises a photoelectric conversion device for converting a brightness level of the light reflected by said object into an electric signal; and*

wherein said device for calculating a remaining exposure time further comprises a device for forming a derivation of said resultant integral value to be used in calculating said remaining exposure time.

24. *A photographing light quantity controller for an endoscope according to claim 20, further comprising a light source shutter adjacent said means for supplying light, said exposure being stopped by closing said light source shutter.*

25. *A photographing light quantity controller for an endoscope according to claim 20, wherein said amplifying system is operable using a plurality of amplification factors, and including a device that automatically switches over said plurality of amplification factors of said amplifying system so that said resultant integral value is amplified by said first amplification factor during said first period of time, by another amplification factor after said first period of time and before said remaining exposure time is calculated, and by said first amplification factor after calculation of said remaining exposure time.*

26. *A photographing light quantity controller for an endoscope according to claim 20, further comprising:*

a comparing device for comparing said resultant integral value with a predetermined reference value; and

means for stopping said exposure upon a first occurrence of one of said integral output voltage value reaching said predetermined reference value and said remaining exposure time elapsing.

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