



US009918713B2

(12) **United States Patent**  
**Zergiebel et al.**

(10) **Patent No.:** **US 9,918,713 B2**  
(45) **Date of Patent:** **Mar. 20, 2018**

(54) **ADAPTER ASSEMBLY FOR INTERCONNECTING ELECTROMECHANICAL SURGICAL DEVICES AND SURGICAL LOADING UNITS, AND SURGICAL SYSTEMS THEREOF**

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(\*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 574 days.

(21) Appl. No.: **14/550,071**

(22) Filed: **Nov. 21, 2014**

(65) **Prior Publication Data**

US 2015/0157320 A1 Jun. 11, 2015

**Related U.S. Application Data**

(60) Provisional application No. 61/913,550, filed on Dec. 9, 2013.

(51) **Int. Cl.**

**A61B 17/072** (2006.01)

**H01R 39/08** (2006.01)

**A61B 17/00** (2006.01)

(52) **U.S. Cl.**

CPC ..... **A61B 17/07207** (2013.01); **H01R 39/08** (2013.01); **A61B 2017/0046** (2013.01); **A61B 2017/00398** (2013.01); **A61B 2017/00473** (2013.01); **A61B 2017/00477** (2013.01); **A61B 2017/00486** (2013.01); **A61B 2017/00734** (2013.01); **A61B 2017/07271** (2013.01);

(Continued)

(58) **Field of Classification Search**

CPC ..... H01R 39/08; A61B 2017/00398; A61B 2017/0046; A61B 2017/00473; A61B 2017/00477; A61B 2017/00486; A61B 2017/00734; A61B 2017/07271; A61B 2017/07285; A61B 17/07207

USPC ..... 227/175.1  
See application file for complete search history.

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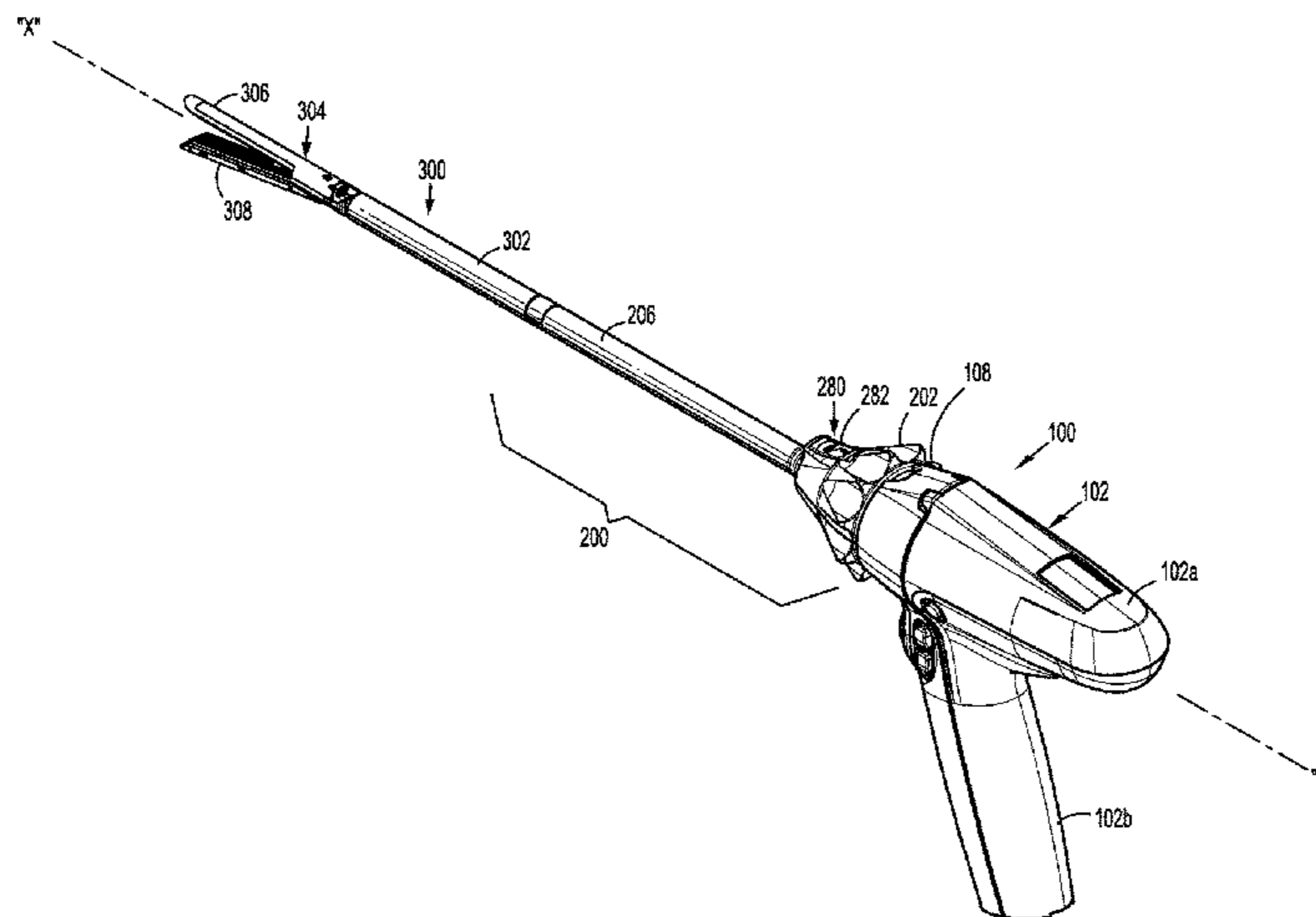
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(57) **ABSTRACT**

The present disclosure relates to adapter assemblies for use with and to electrically and mechanically interconnect electromechanical surgical devices and surgical loading units, and to surgical systems including hand held electromechanical surgical devices and adapter assemblies for connecting surgical loading units to the hand held electromechanical surgical devices.

**13 Claims, 27 Drawing Sheets**



(52) **U.S. Cl.**  
 CPC ..... A61B 2017/07285 (2013.01); Y10T  
 74/19614 (2015.01)

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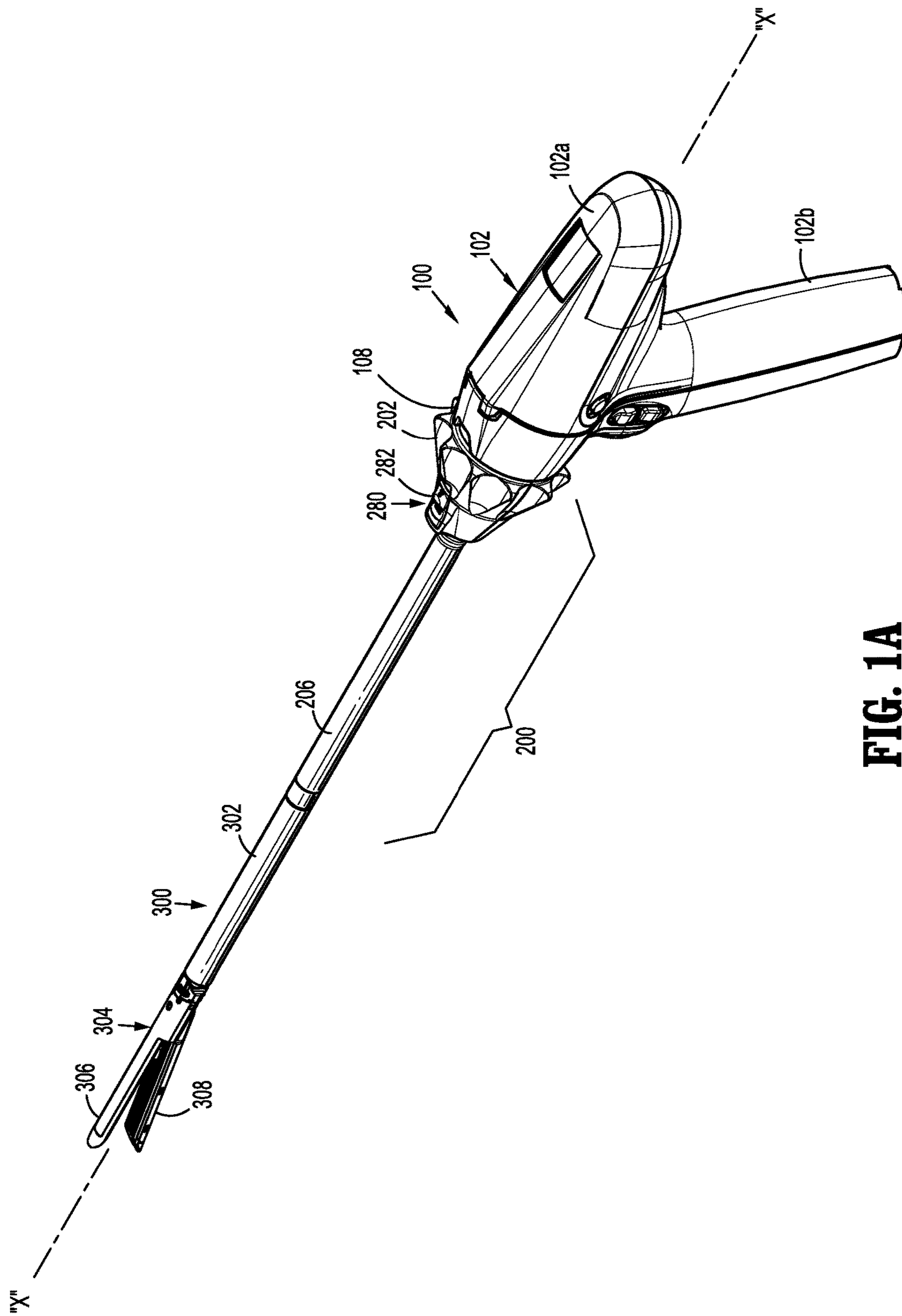
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**FIG. 1A**

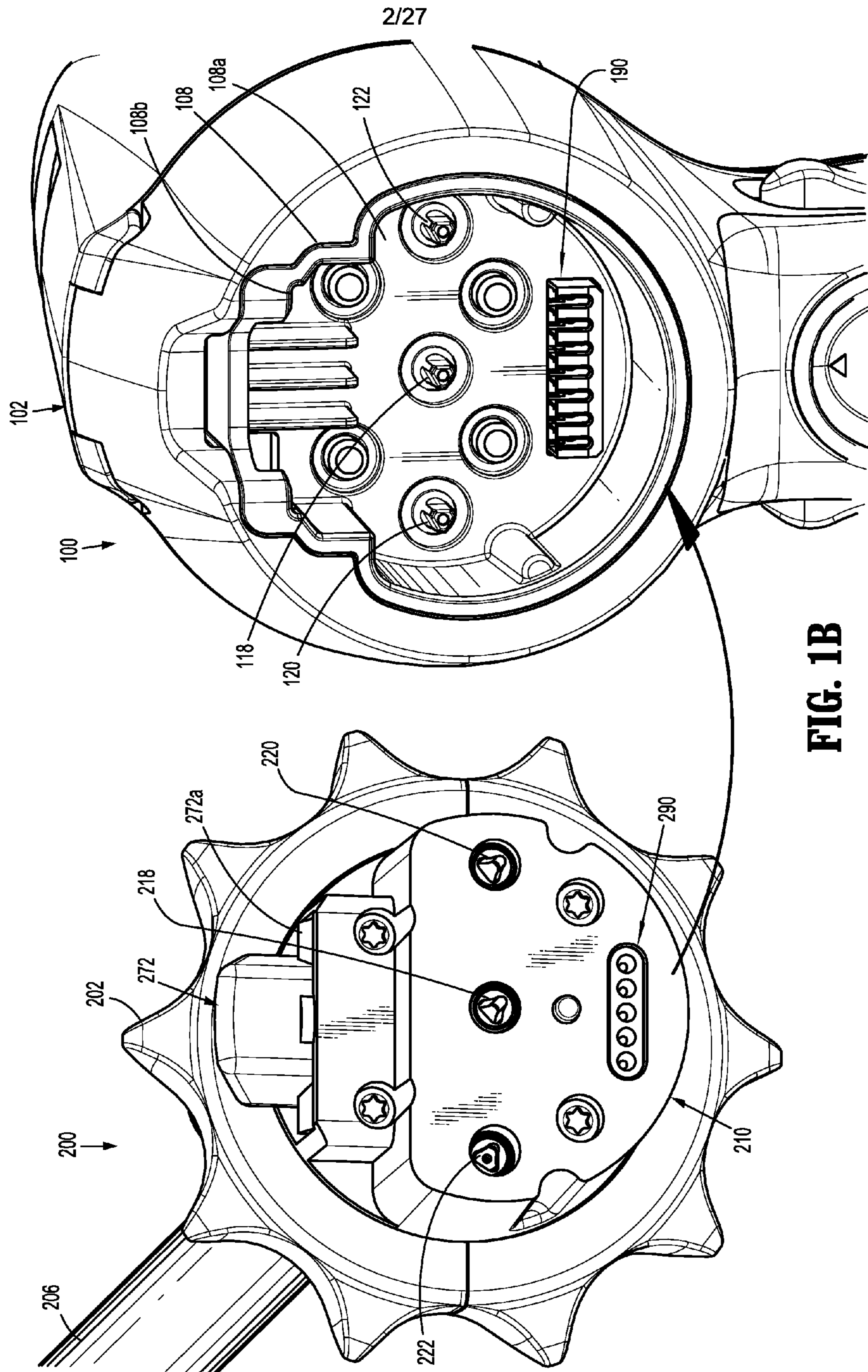
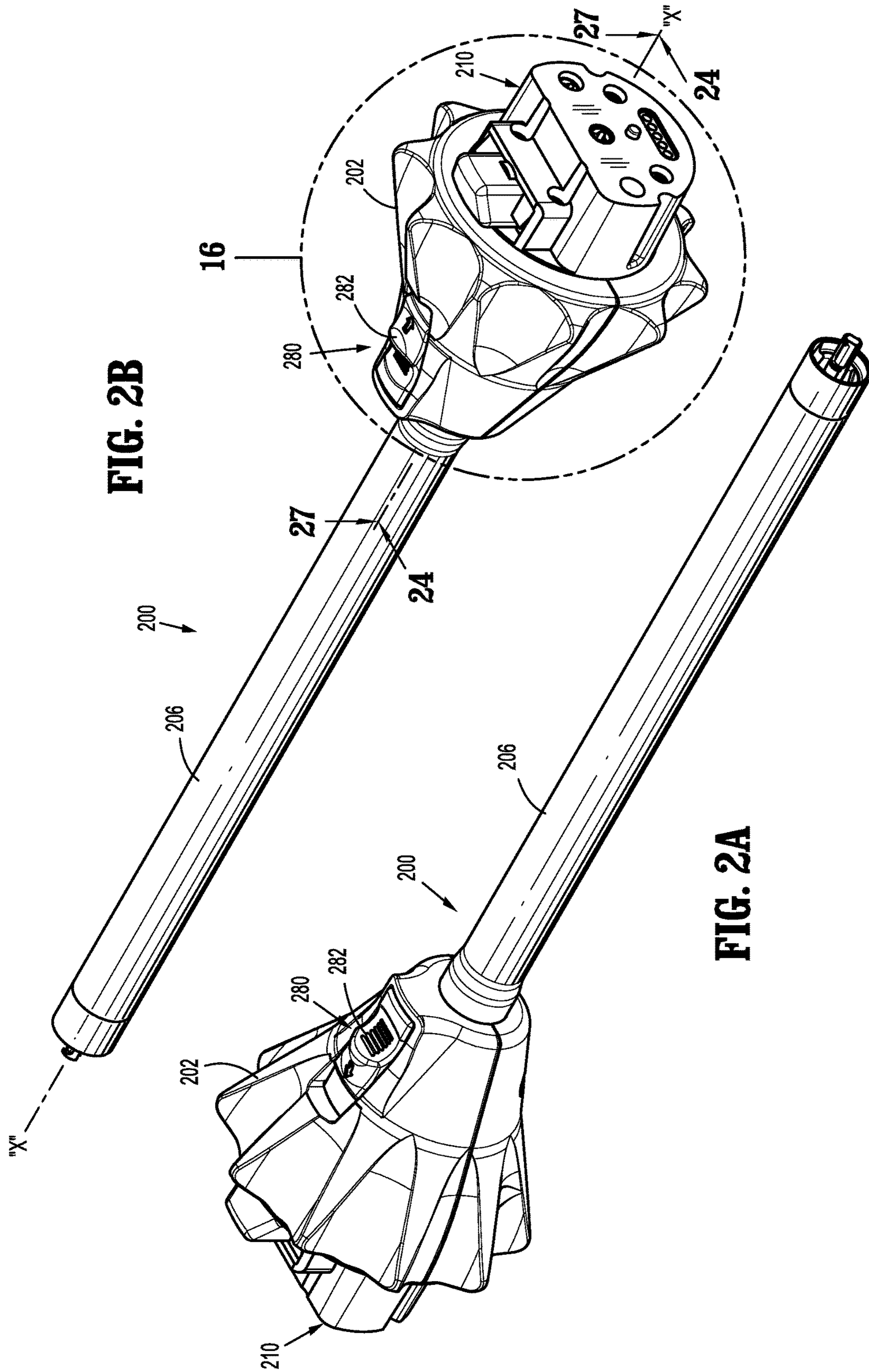


FIG. 1B



**FIG. 2B**

**FIG. 2A**



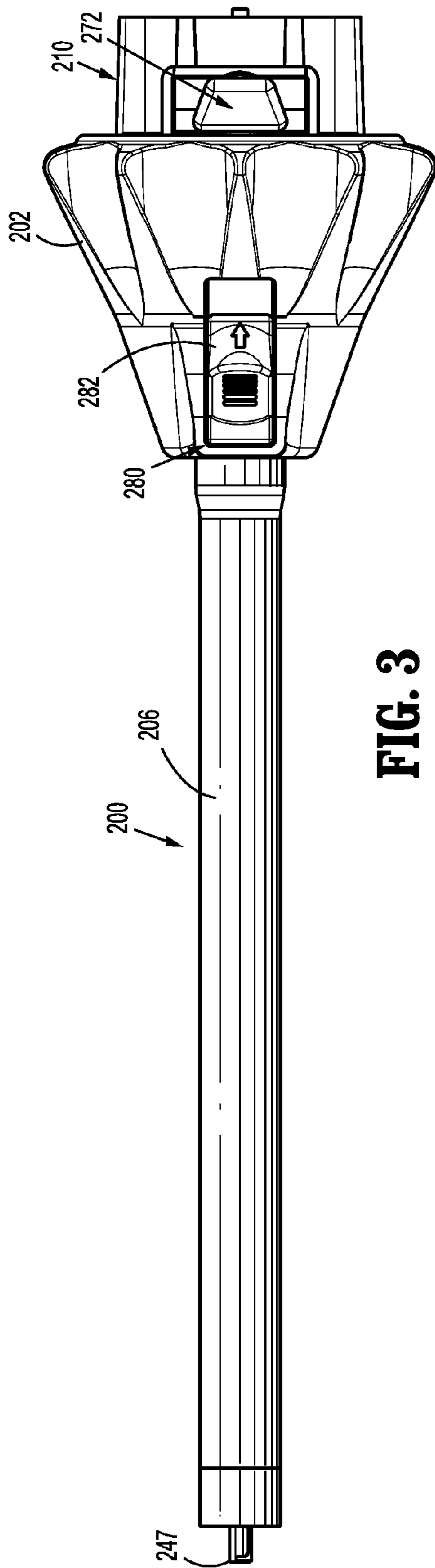


FIG. 3

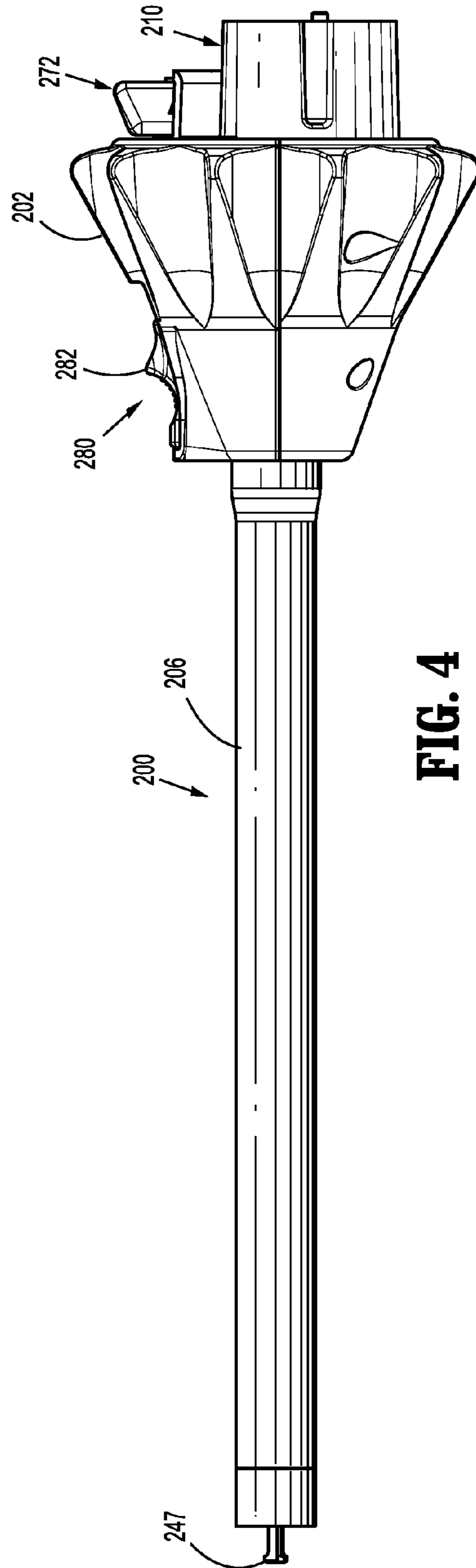
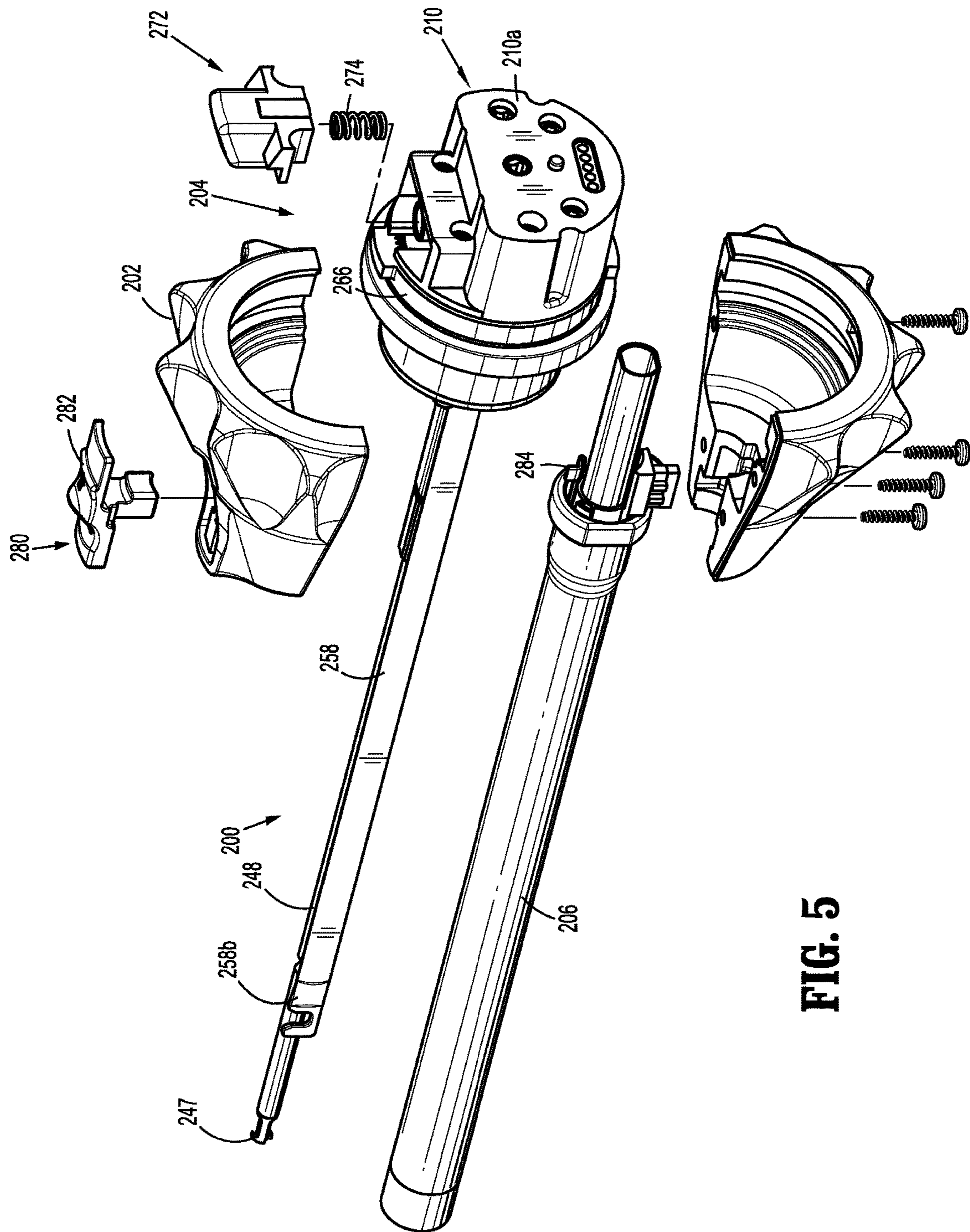
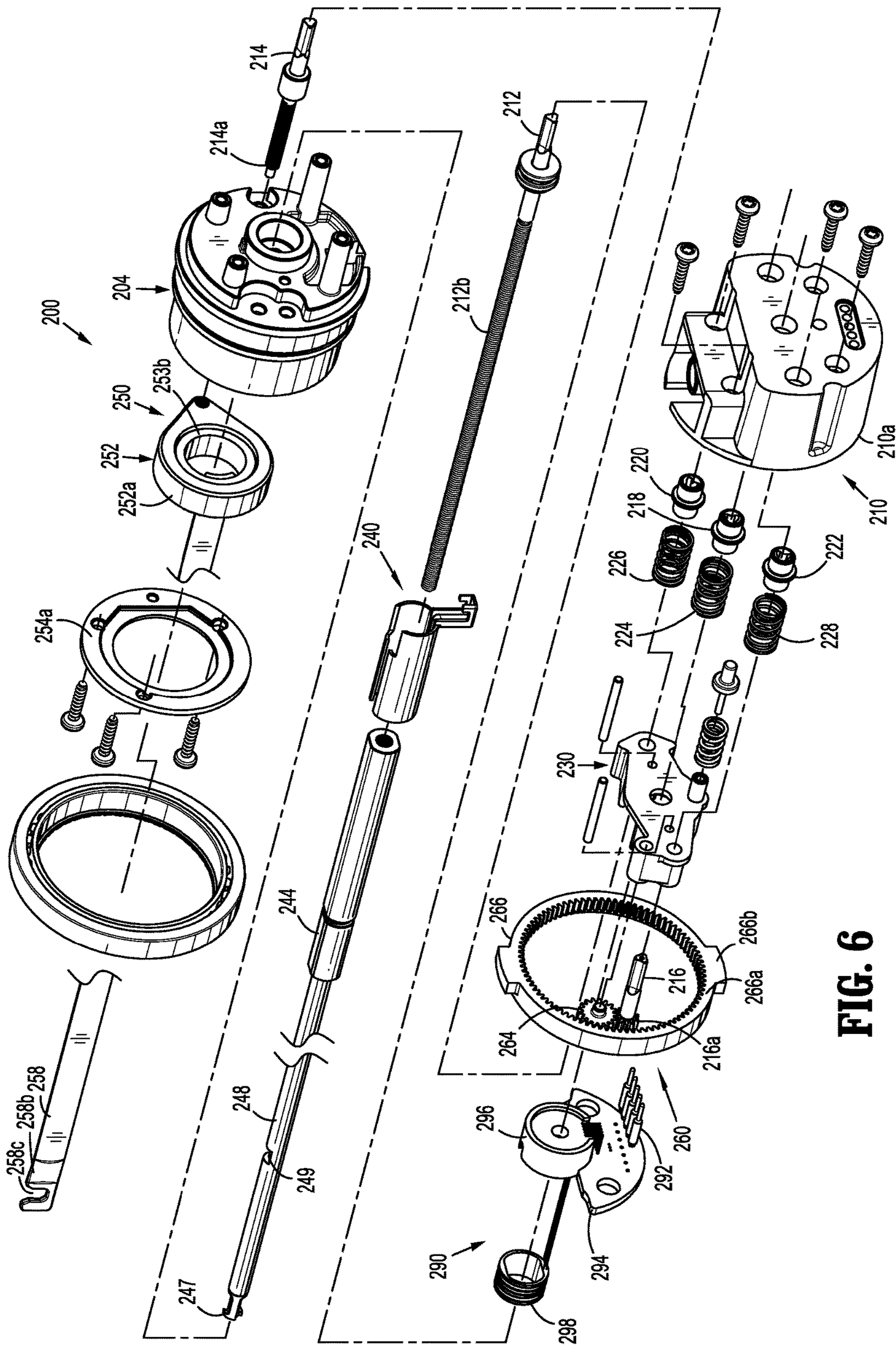


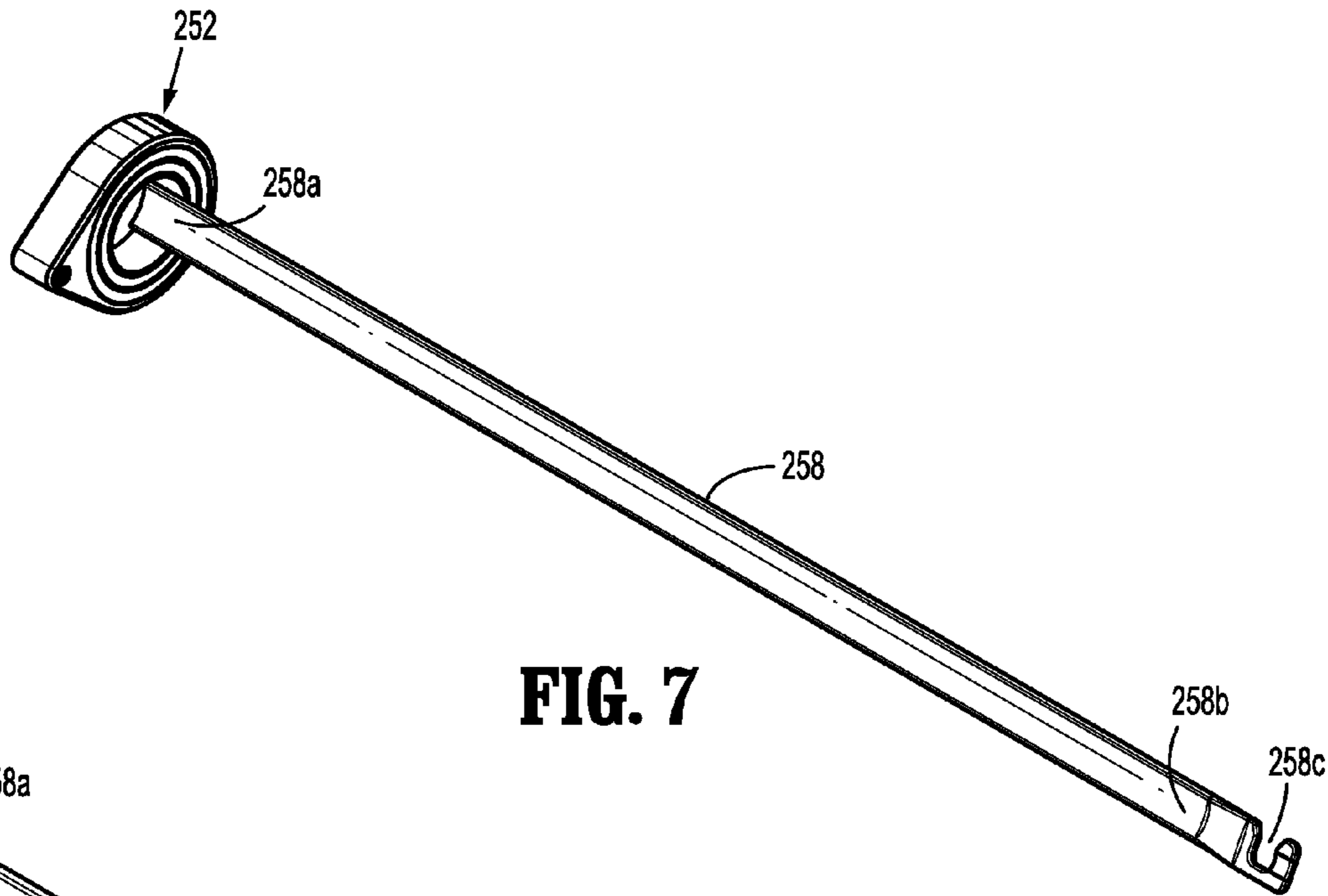
FIG. 4



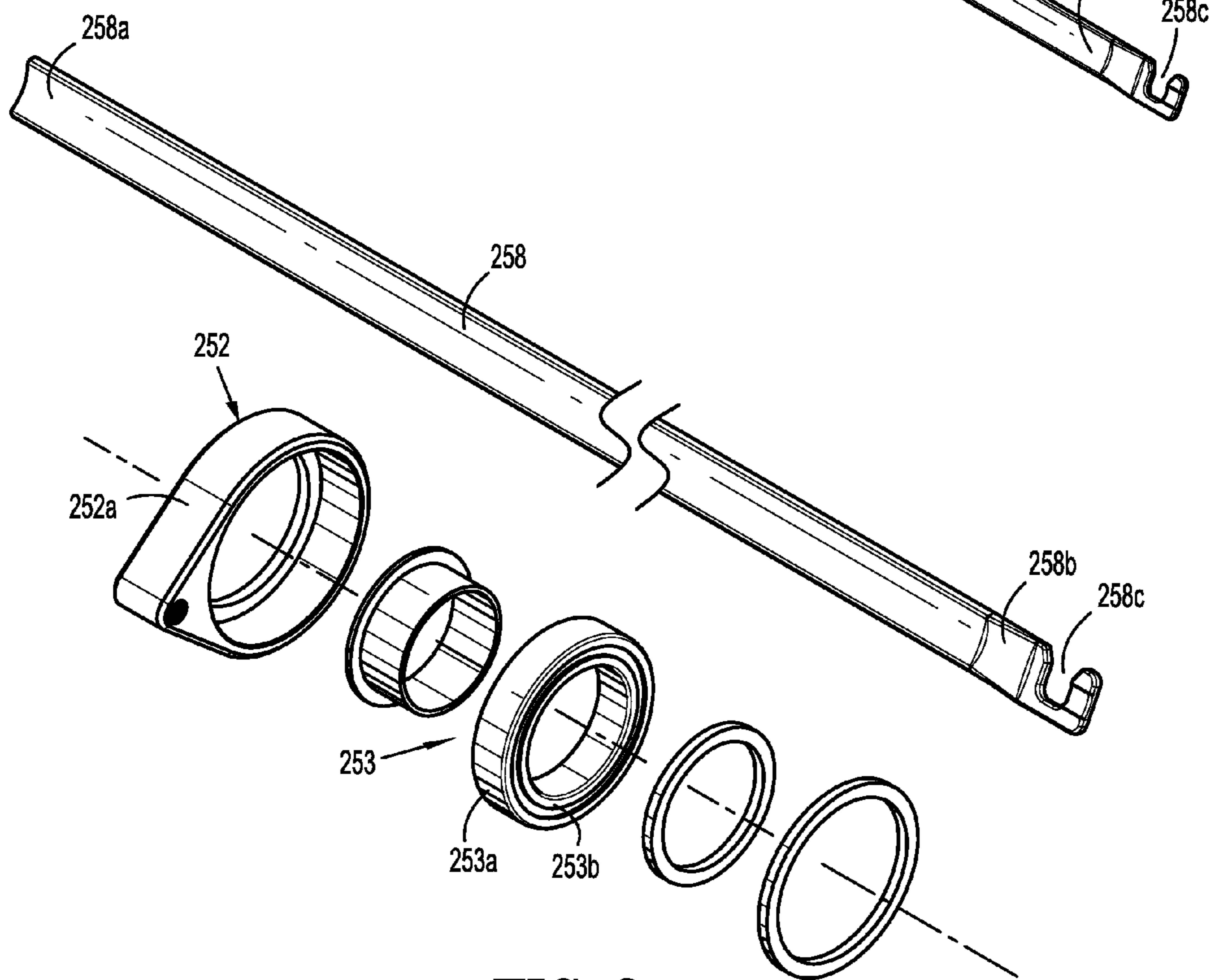
**FIG. 5**



**FIG. 6**



**FIG. 7**



**FIG. 8**

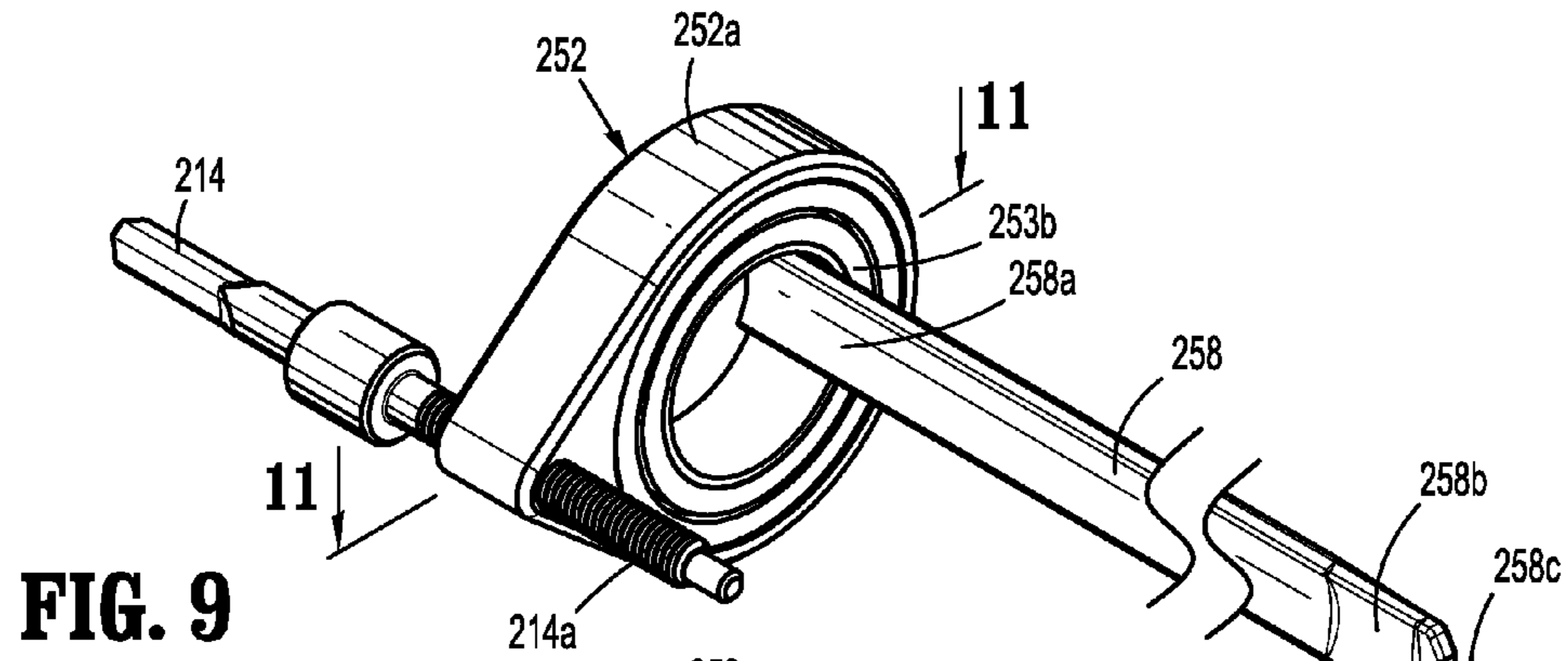


FIG. 9

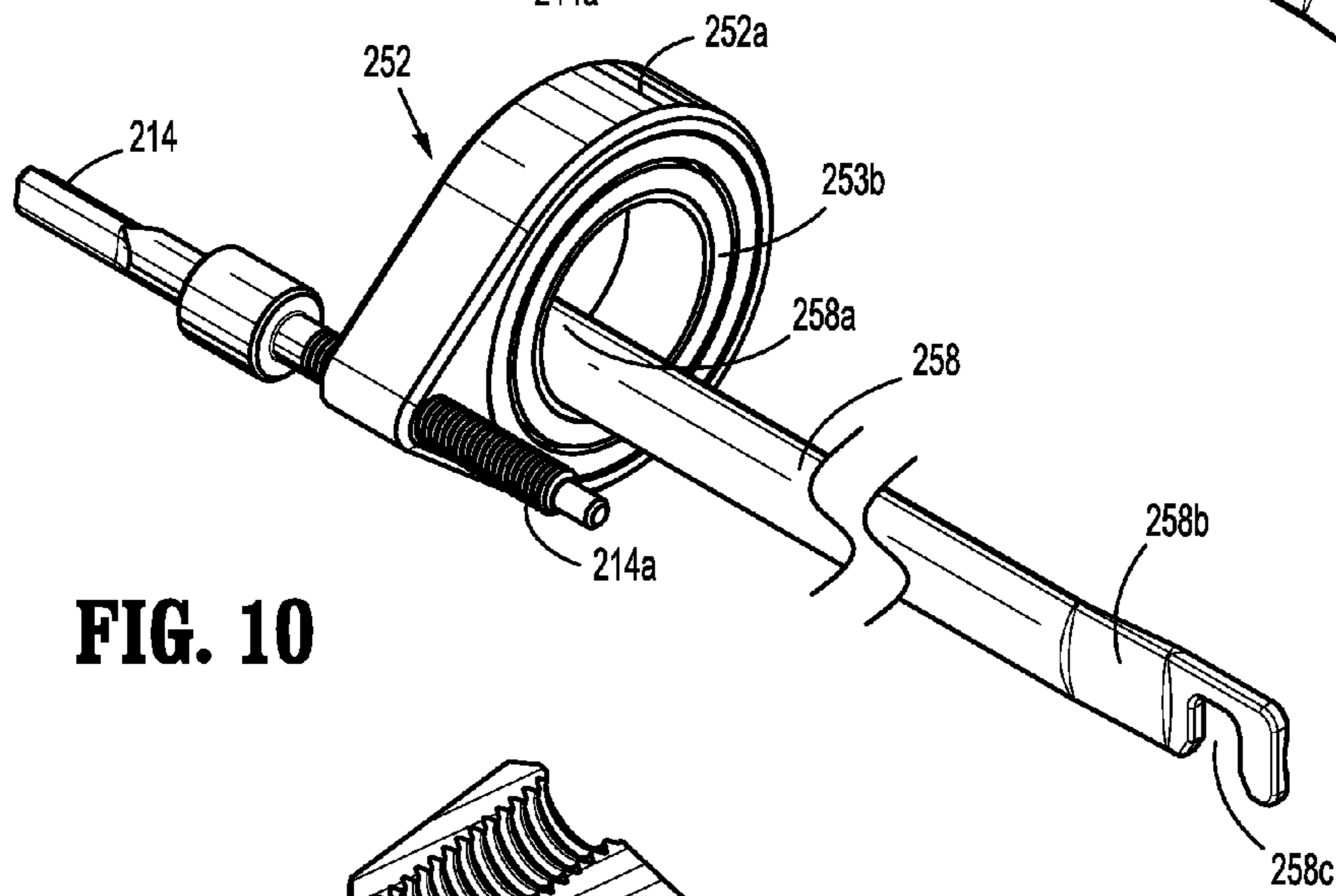


FIG. 10

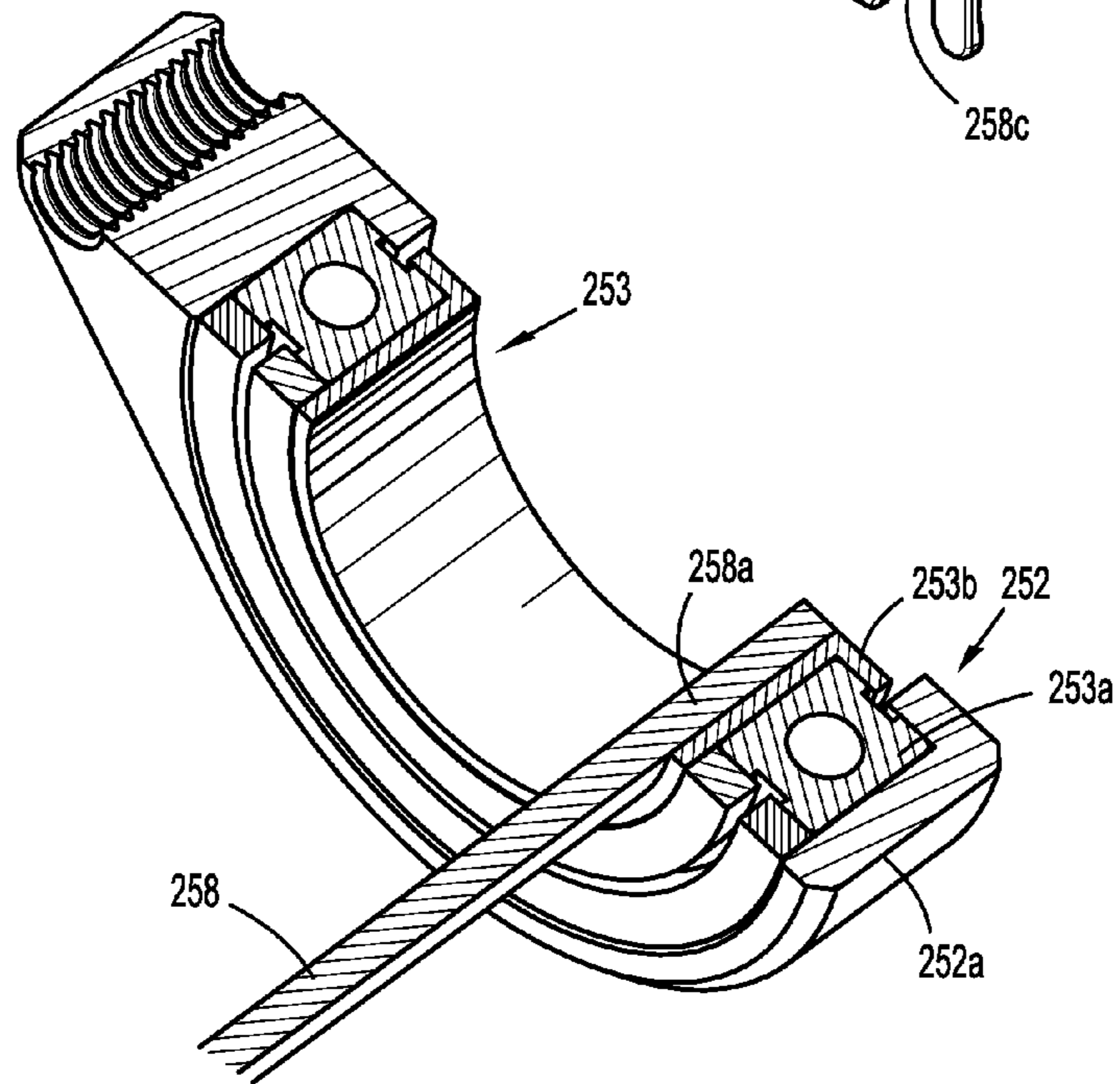
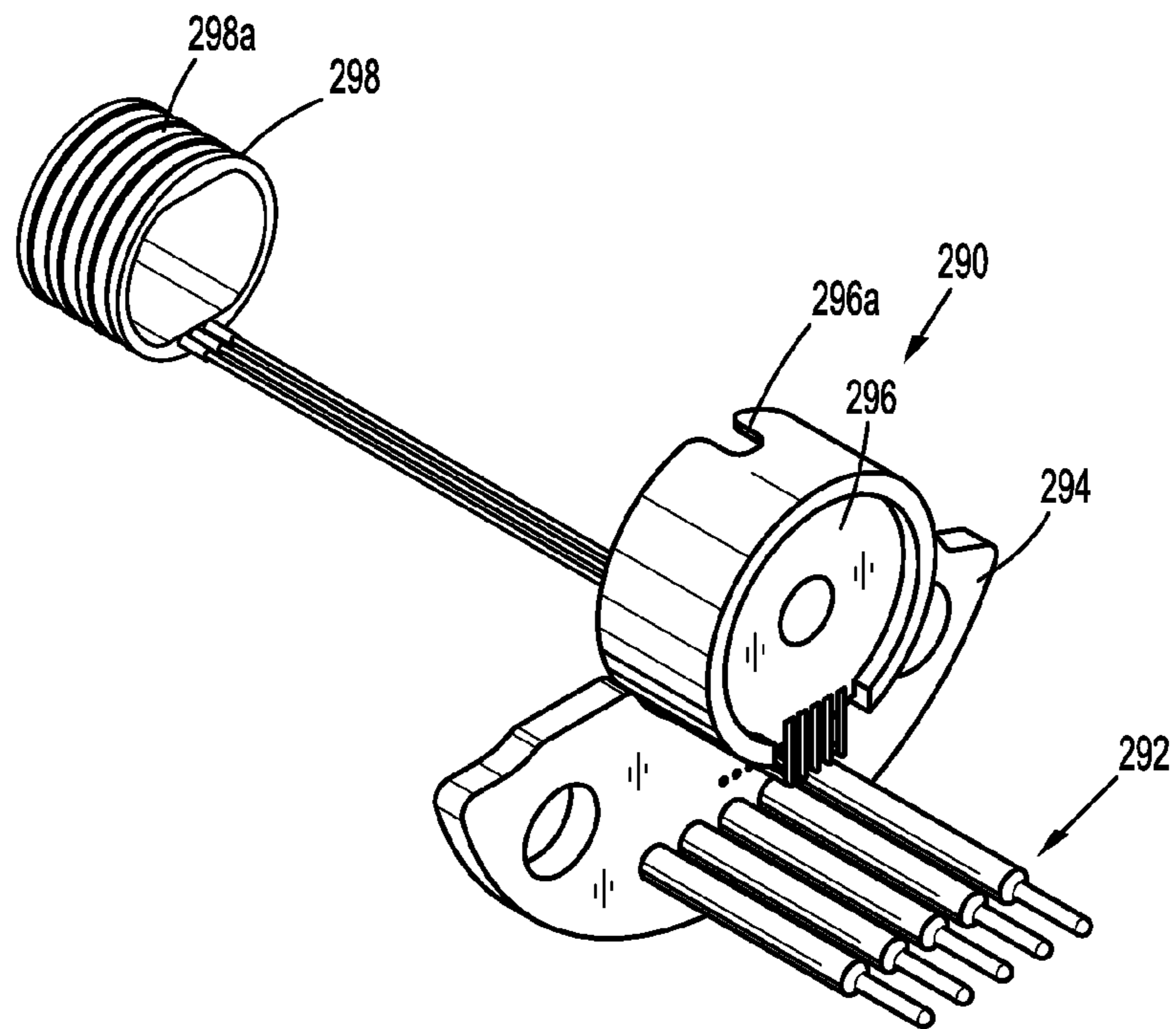
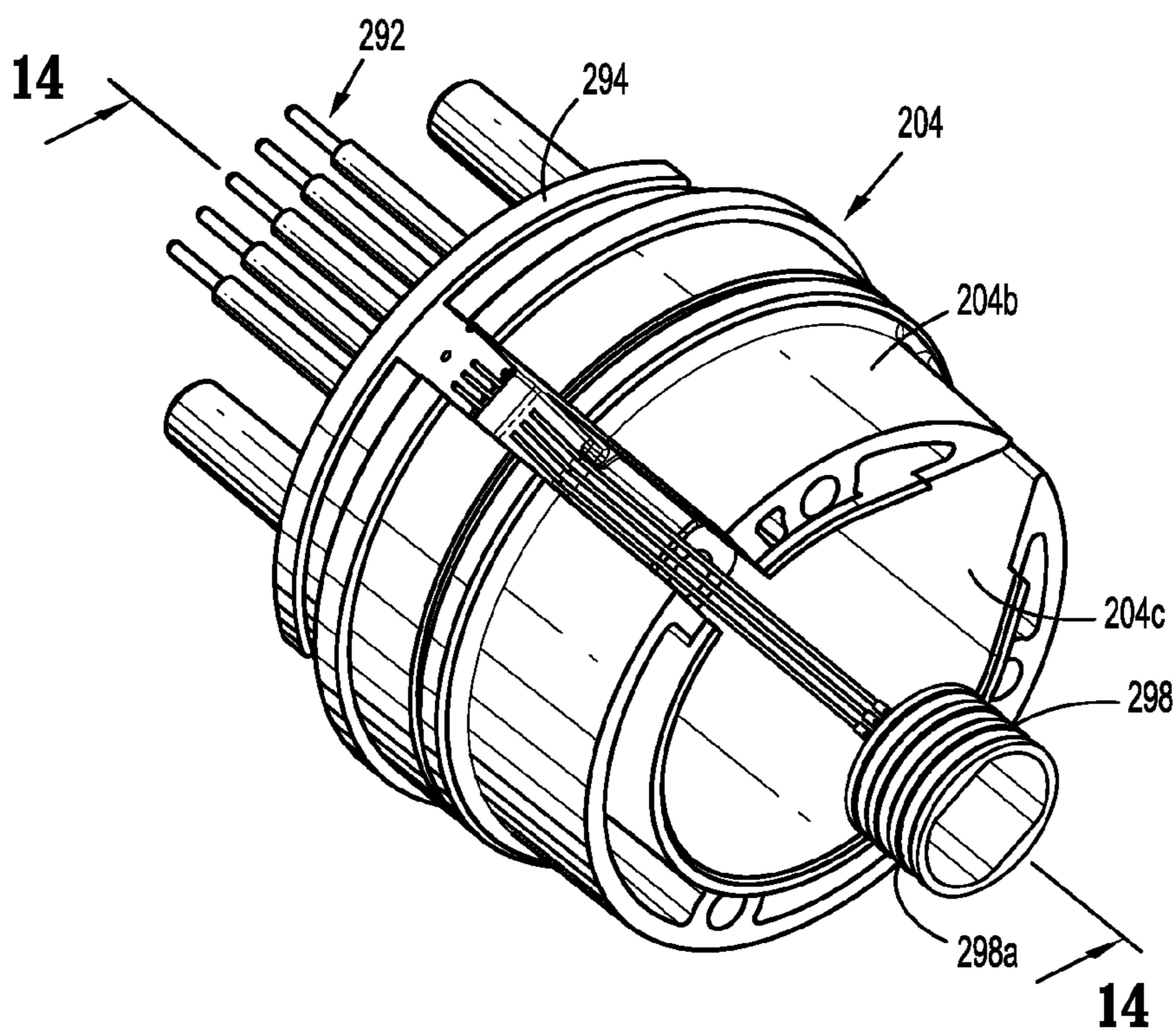


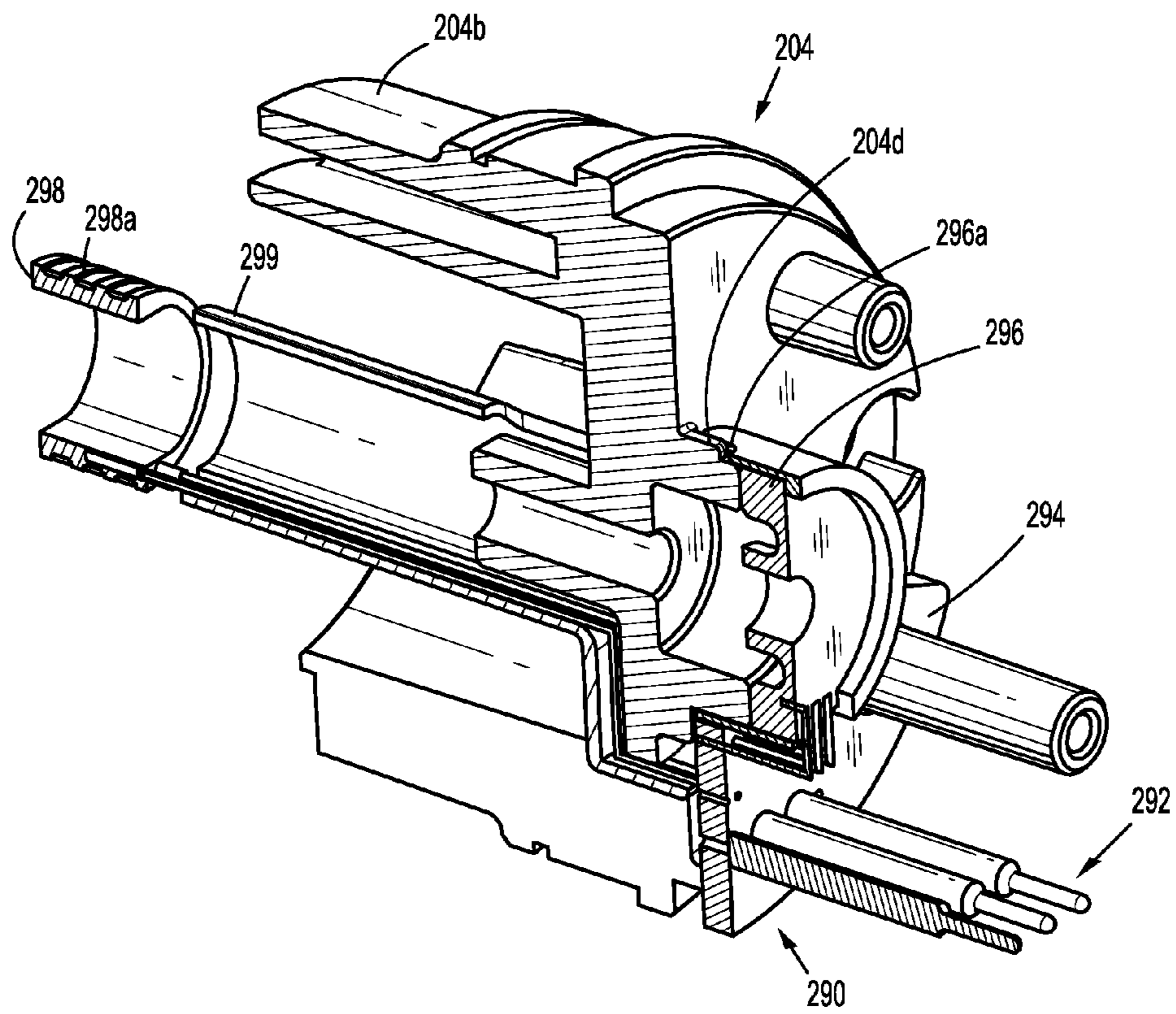
FIG. 11



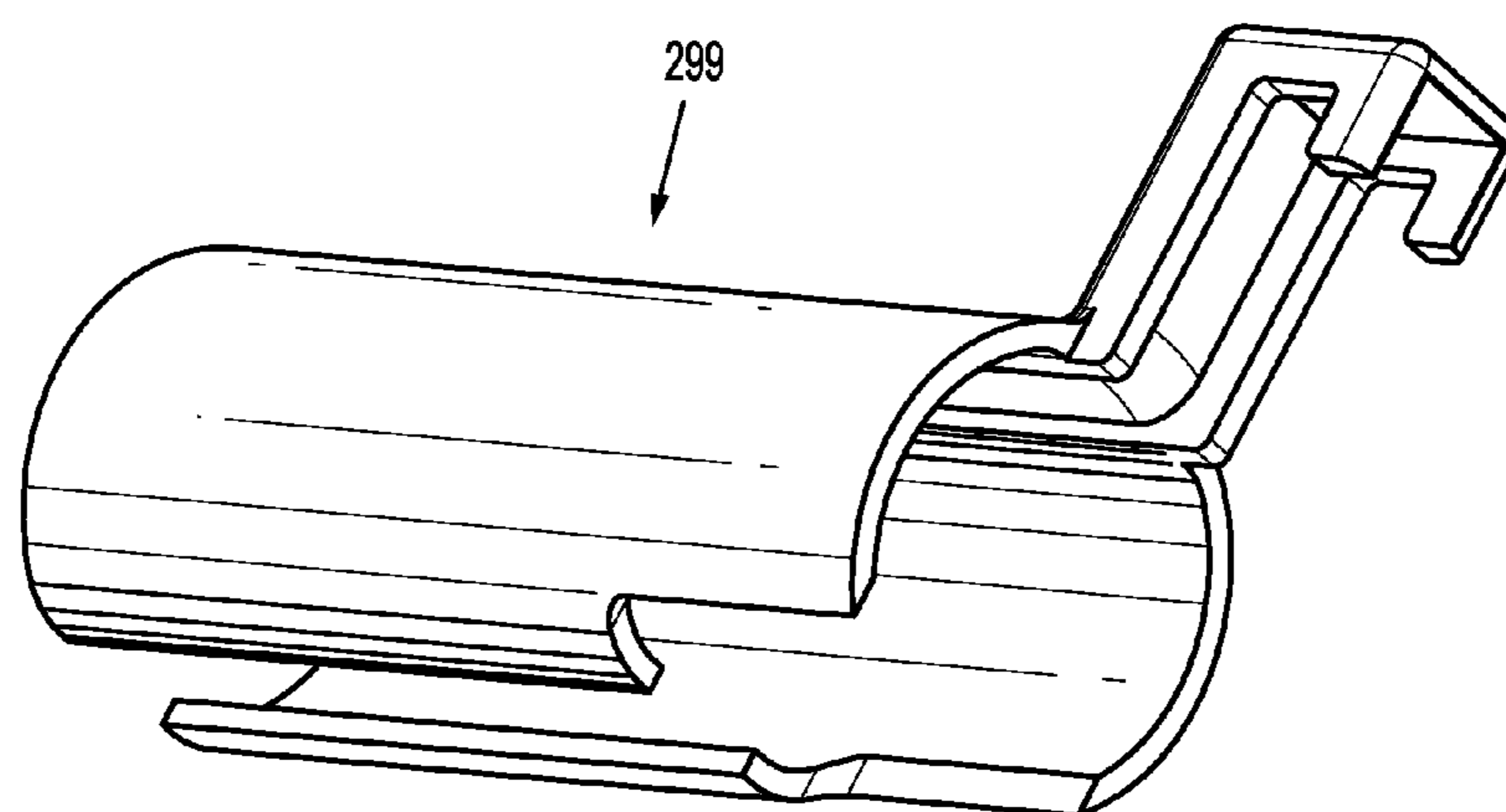
**FIG. 12**



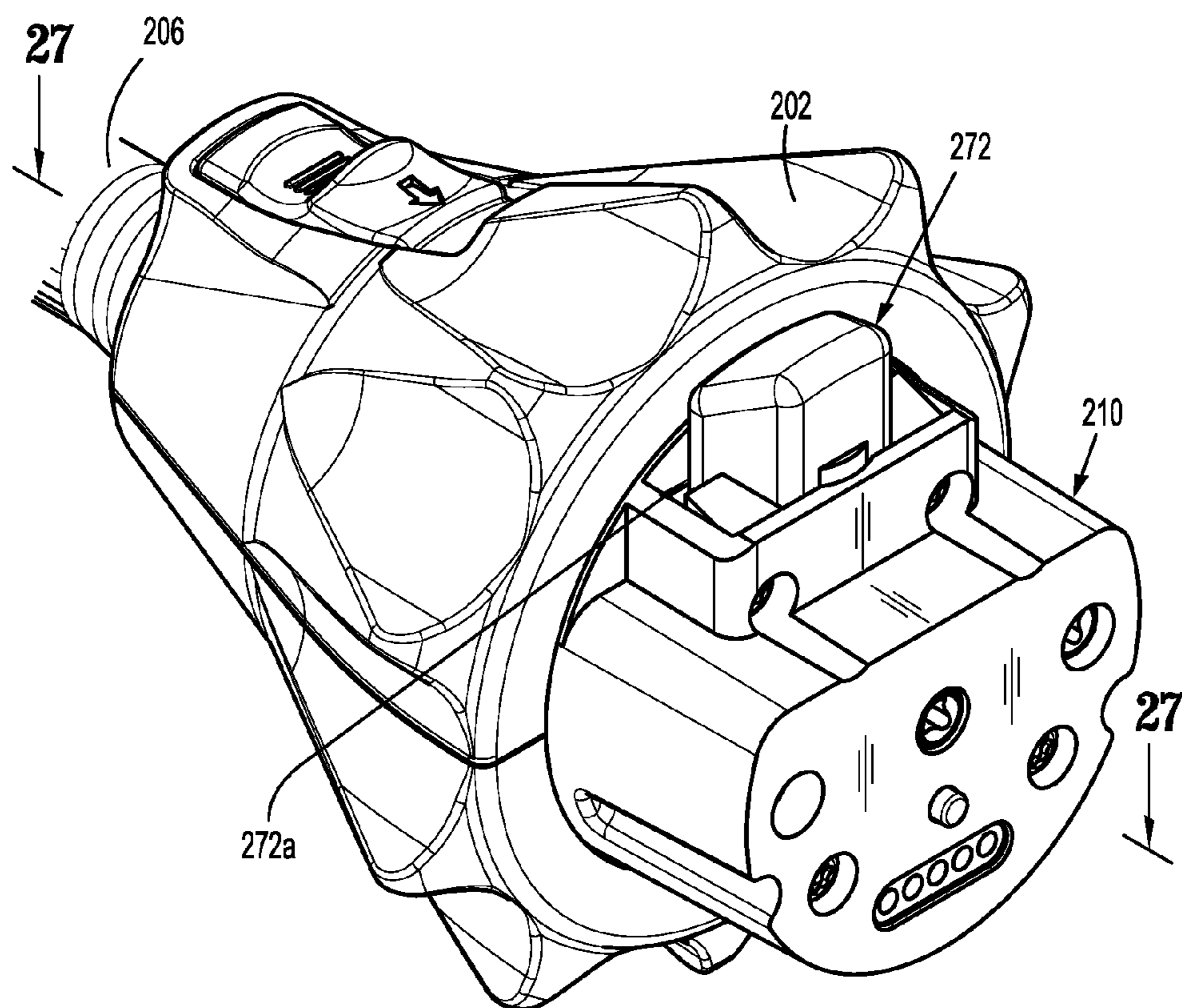
**FIG. 13**



**FIG. 14**

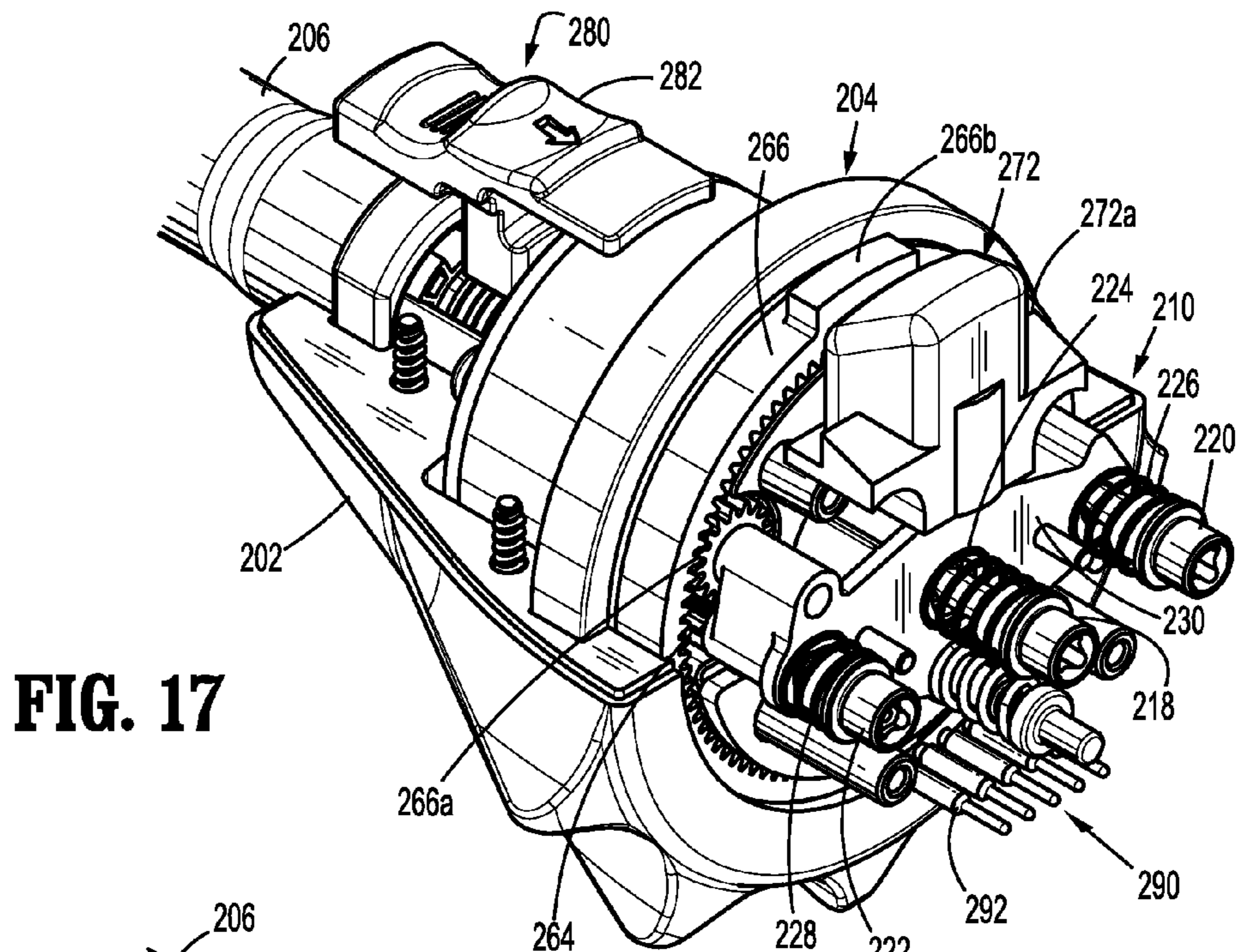


**FIG. 15**

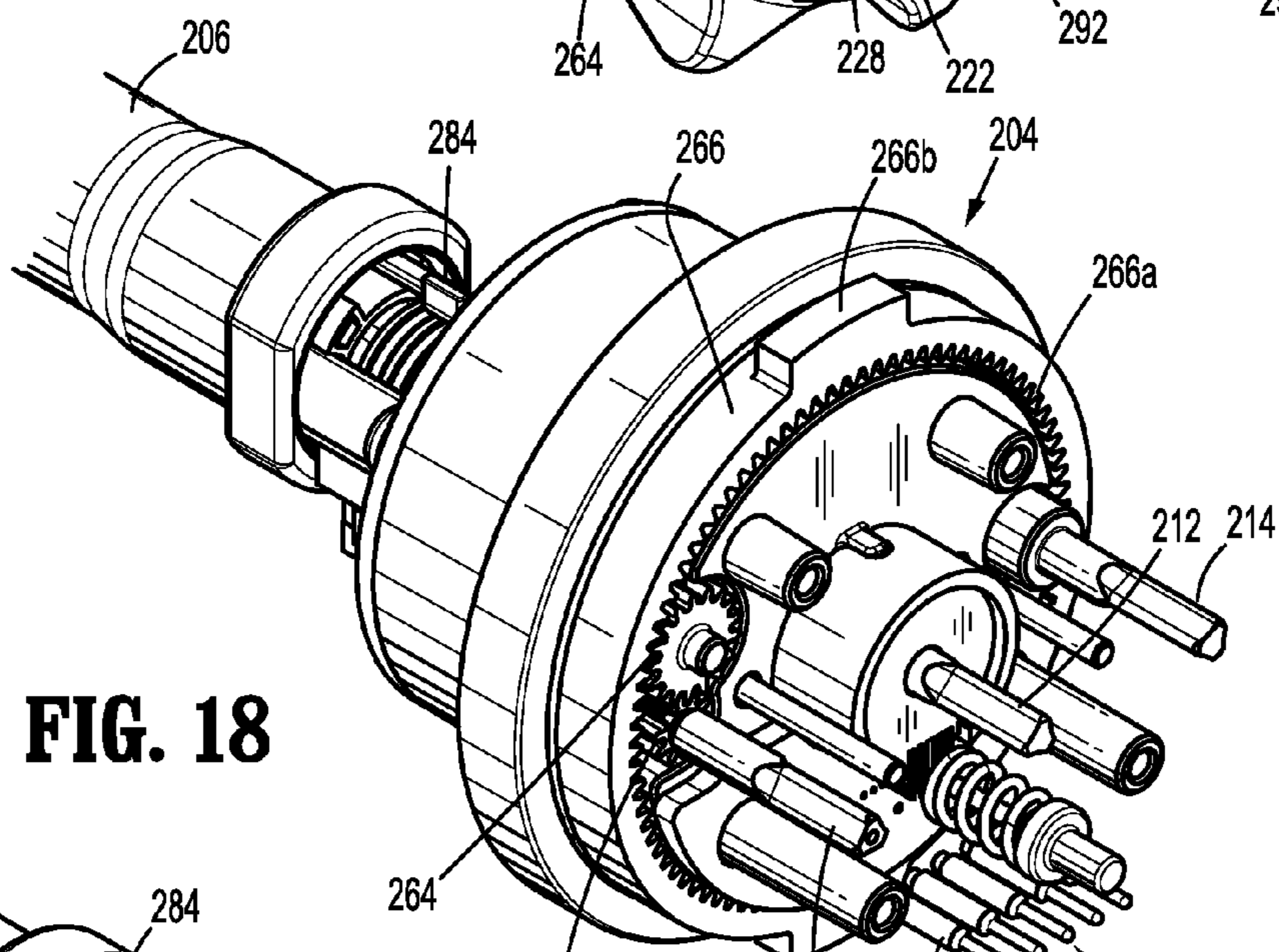


**FIG. 16**

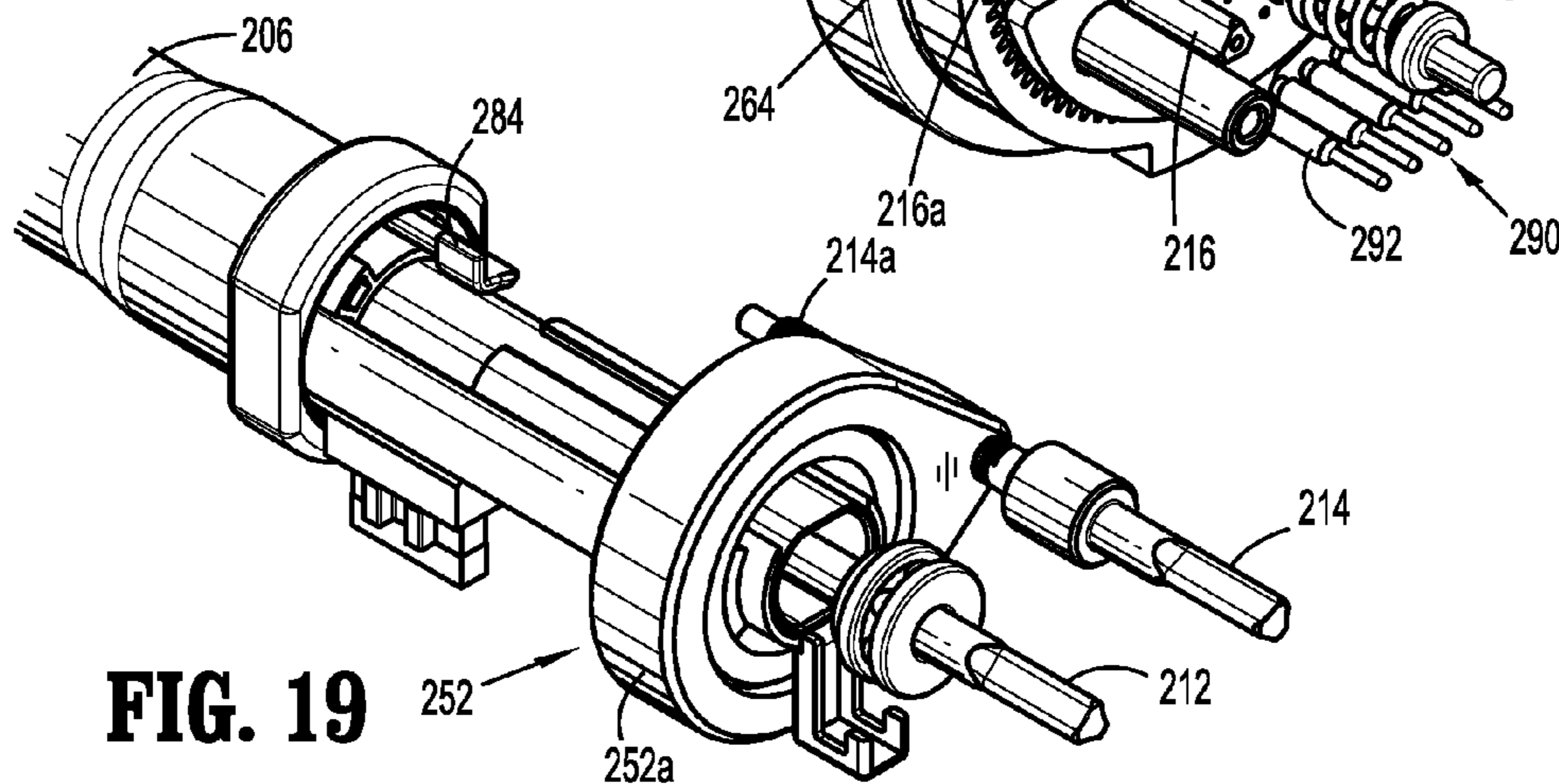




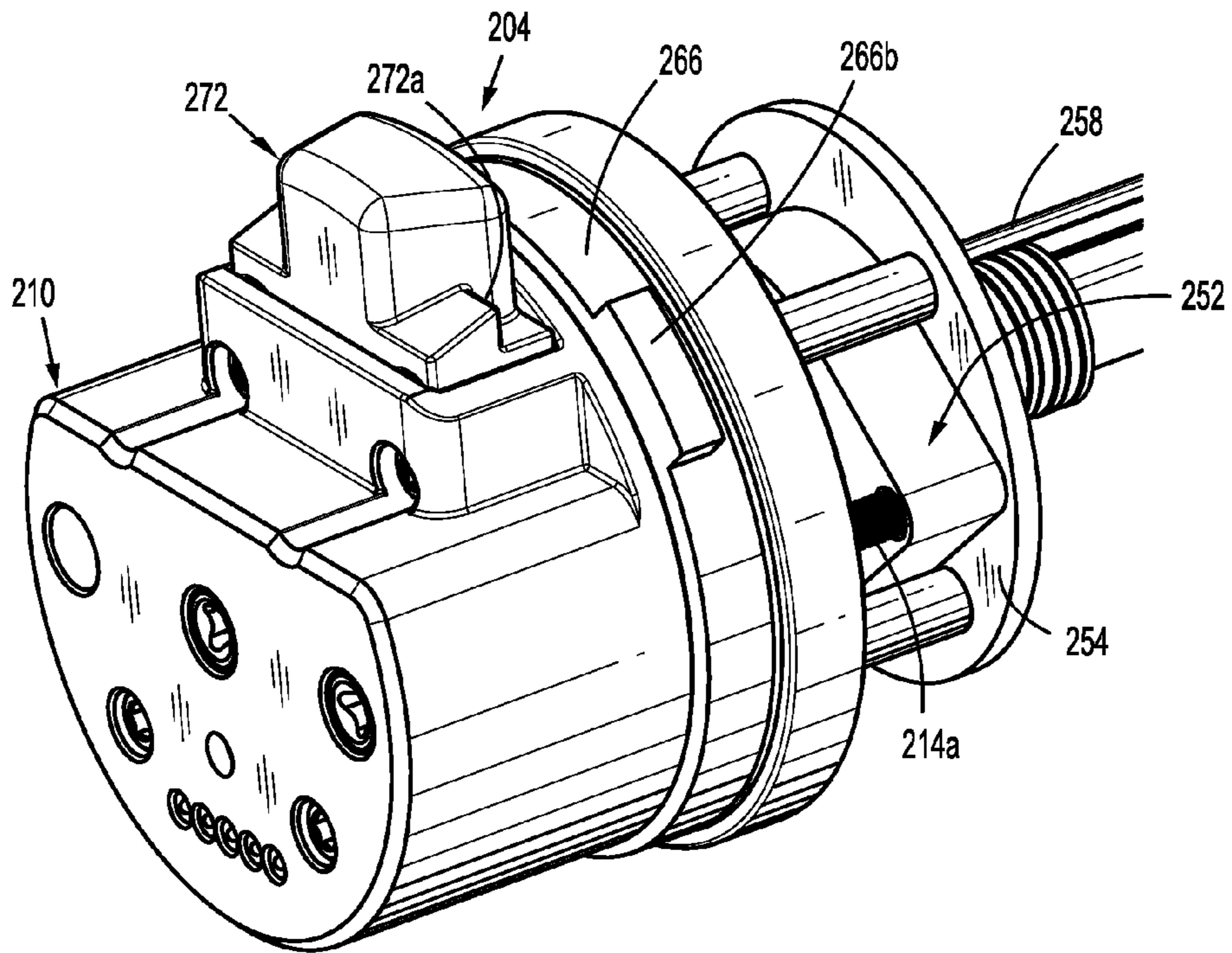
**FIG. 17**



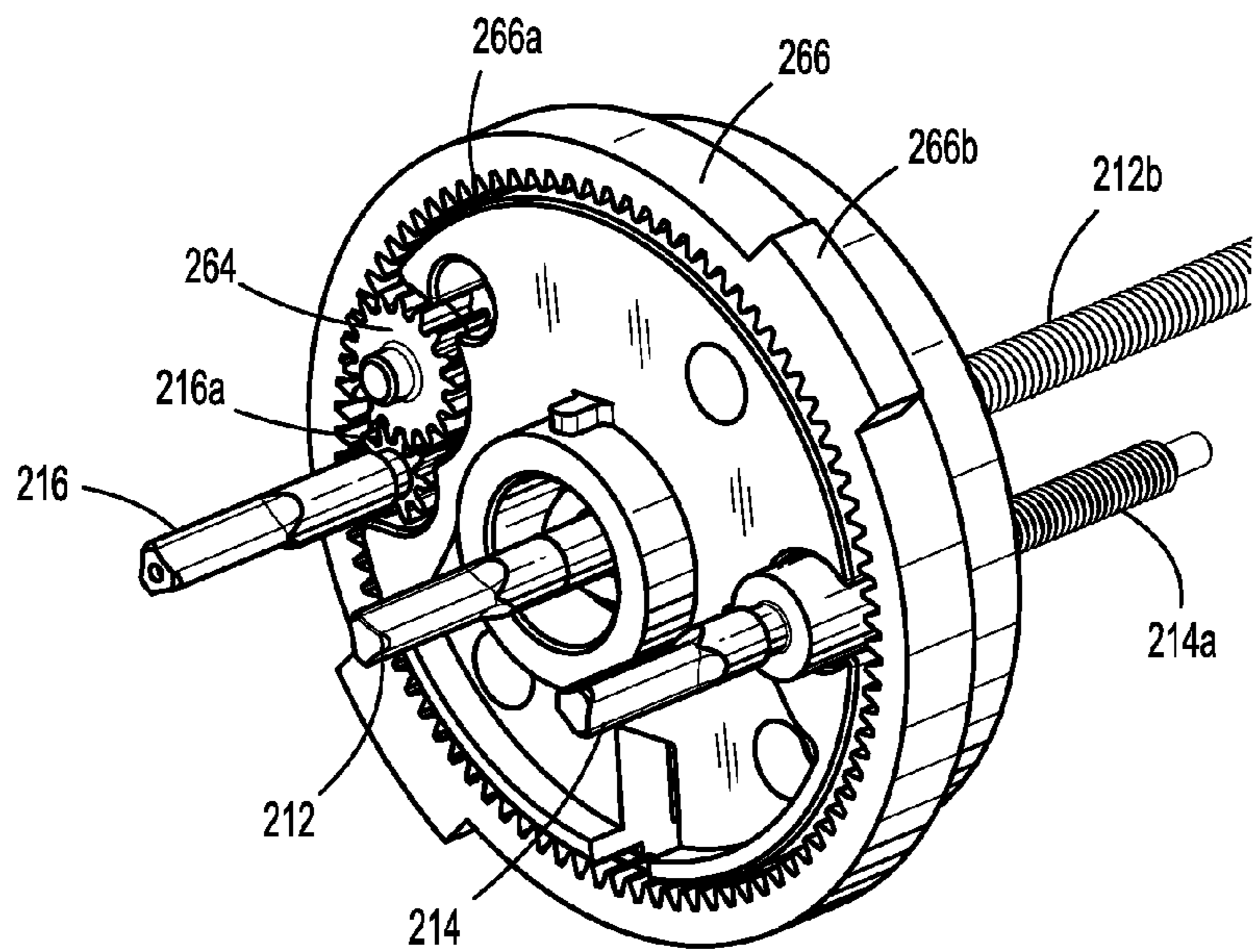
**FIG. 18**



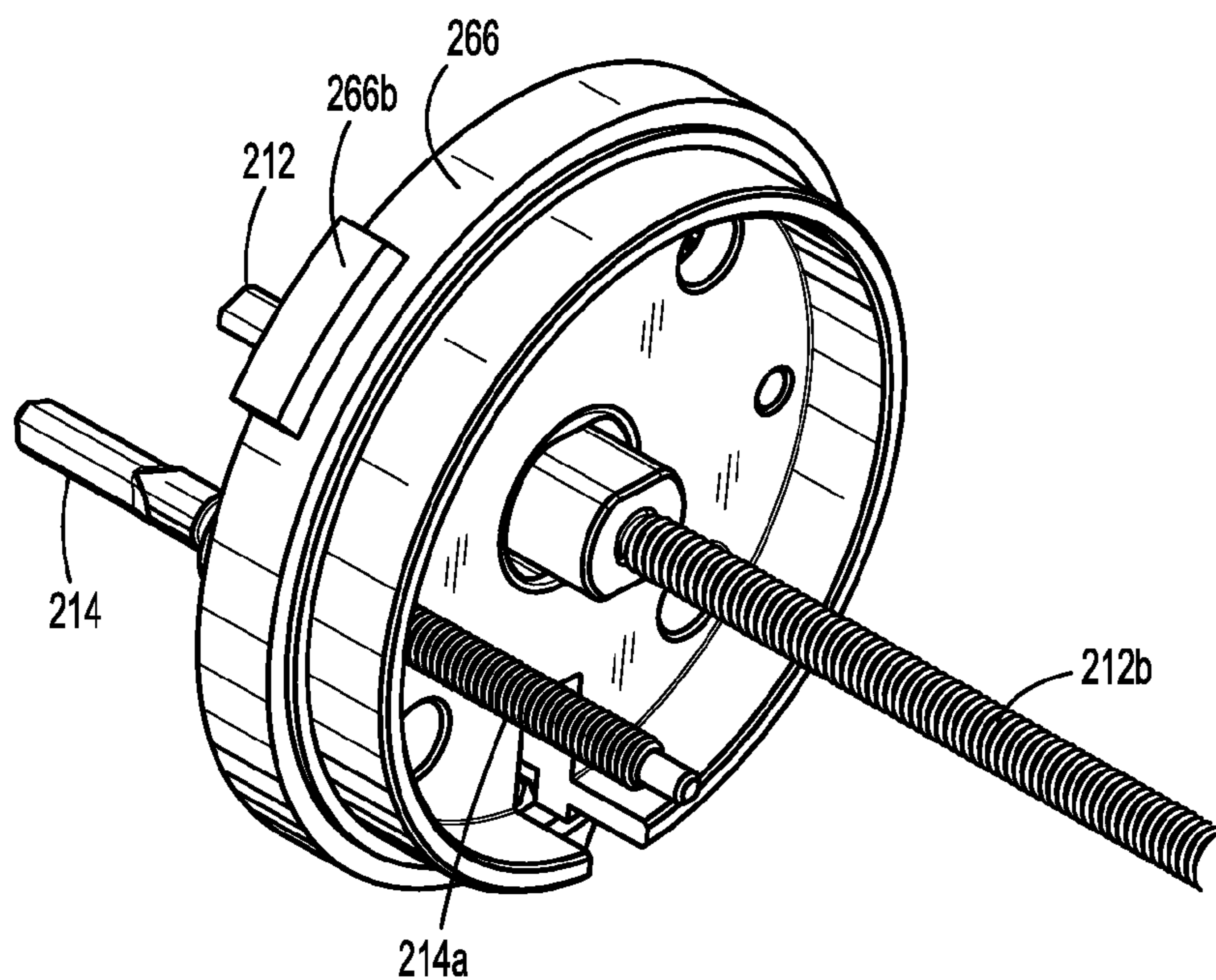
**FIG. 19**



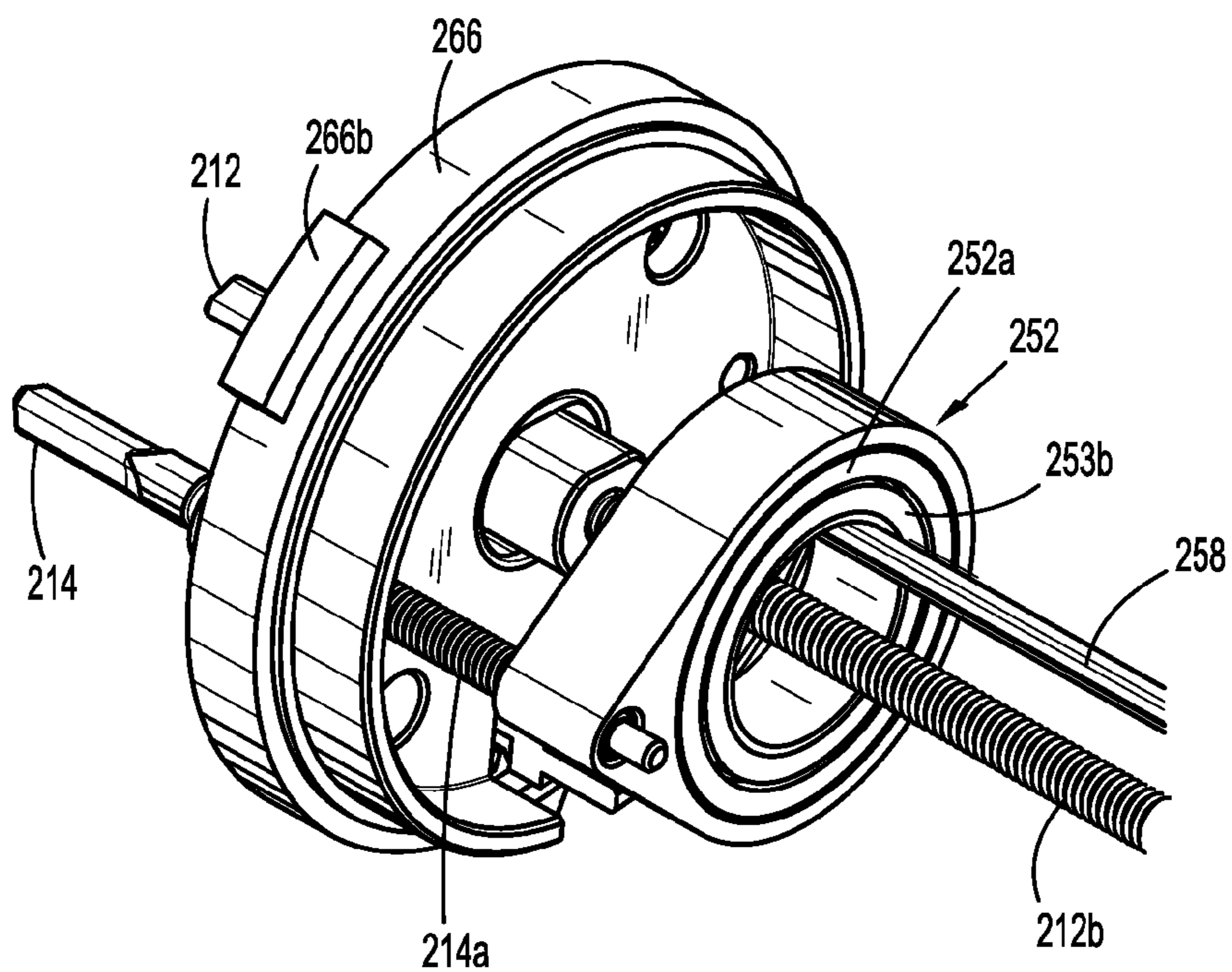
**FIG. 20**



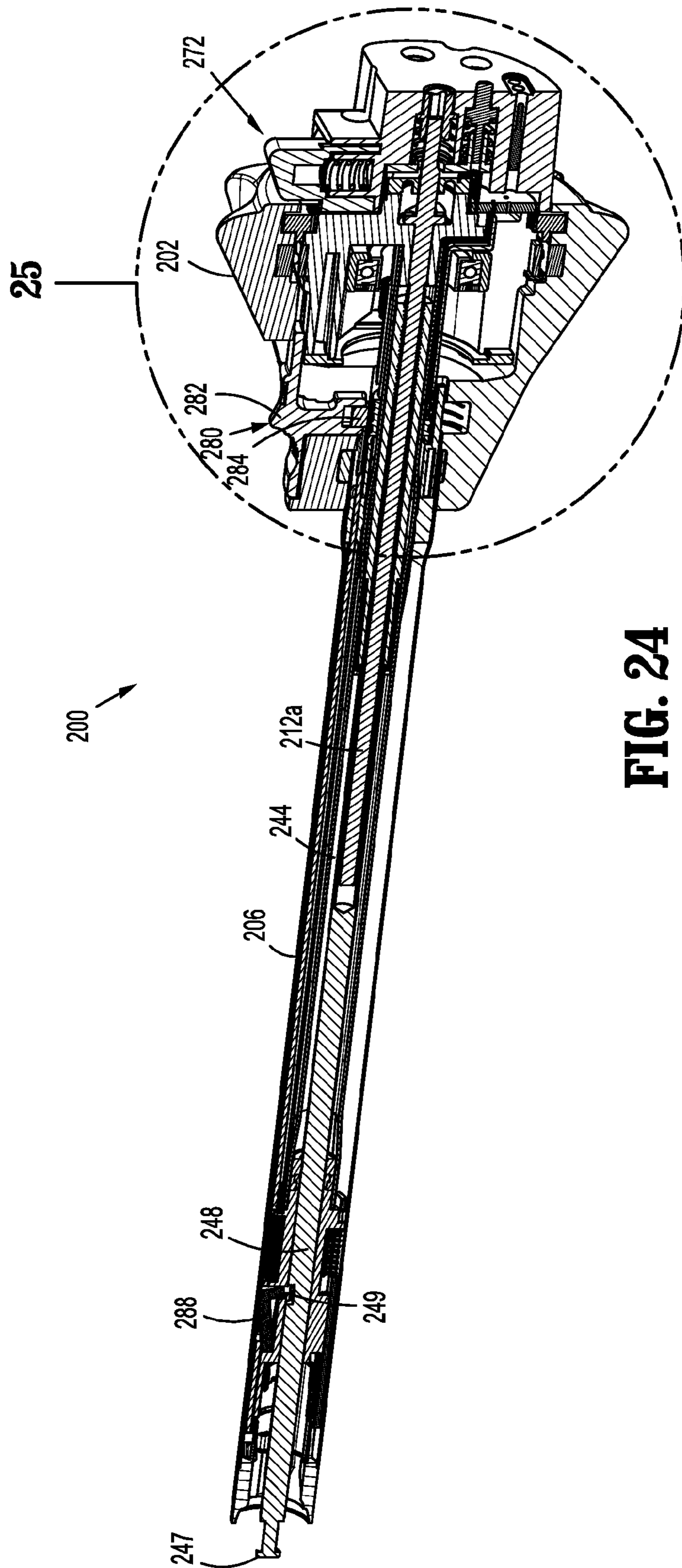
**FIG. 21**



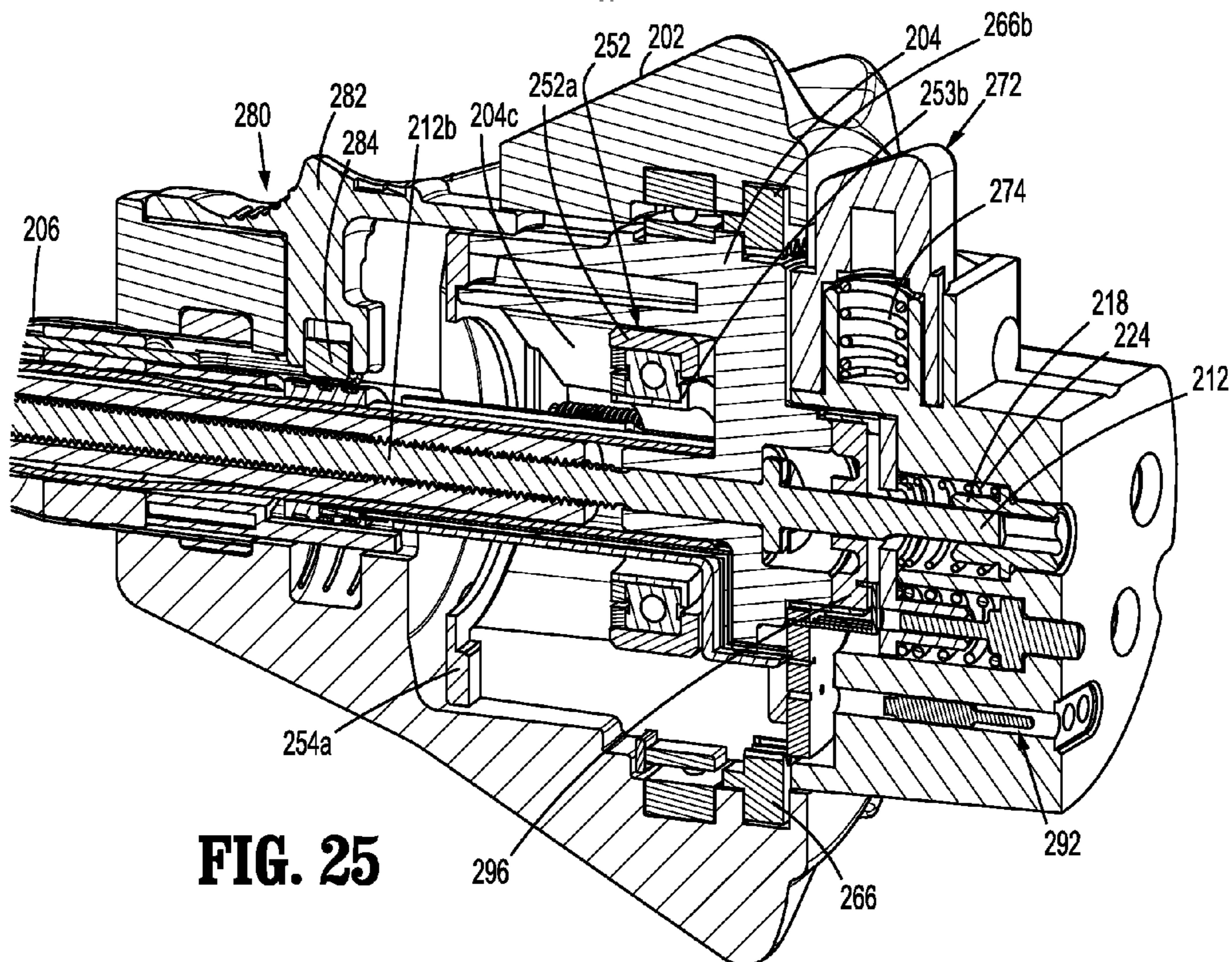
**FIG. 22**



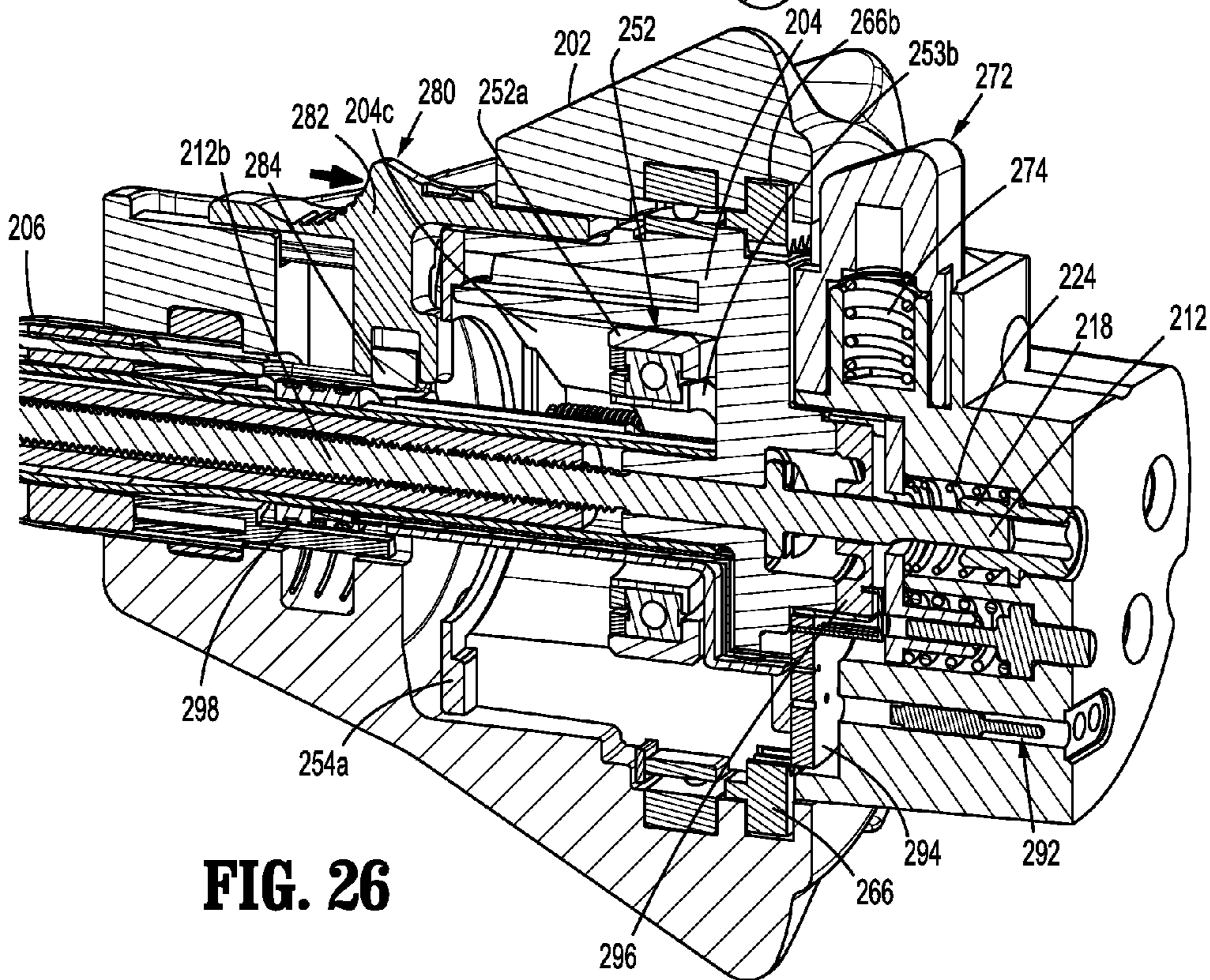
**FIG. 23**



**FIG. 24**



**FIG. 25**



**FIG. 26**

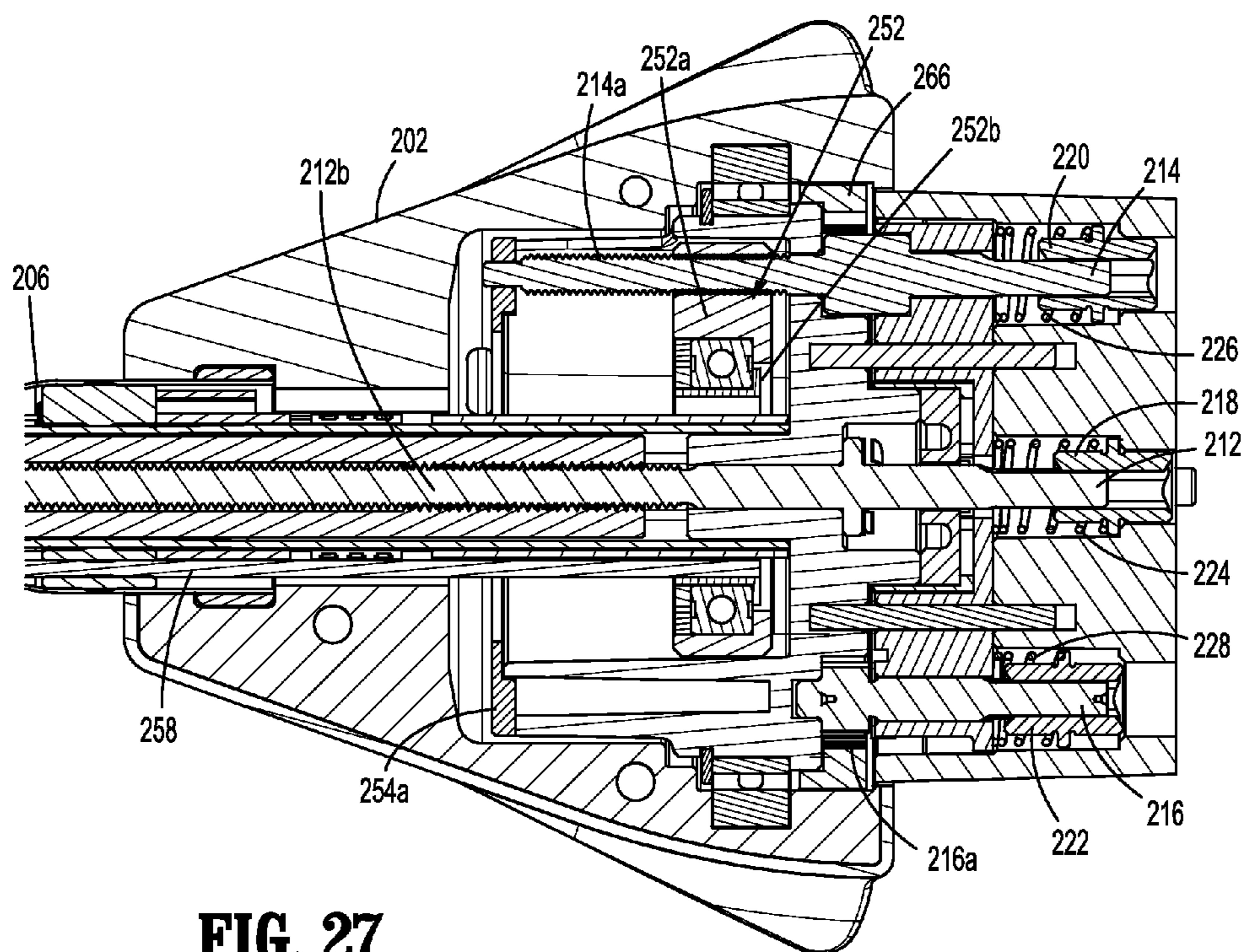


FIG. 27

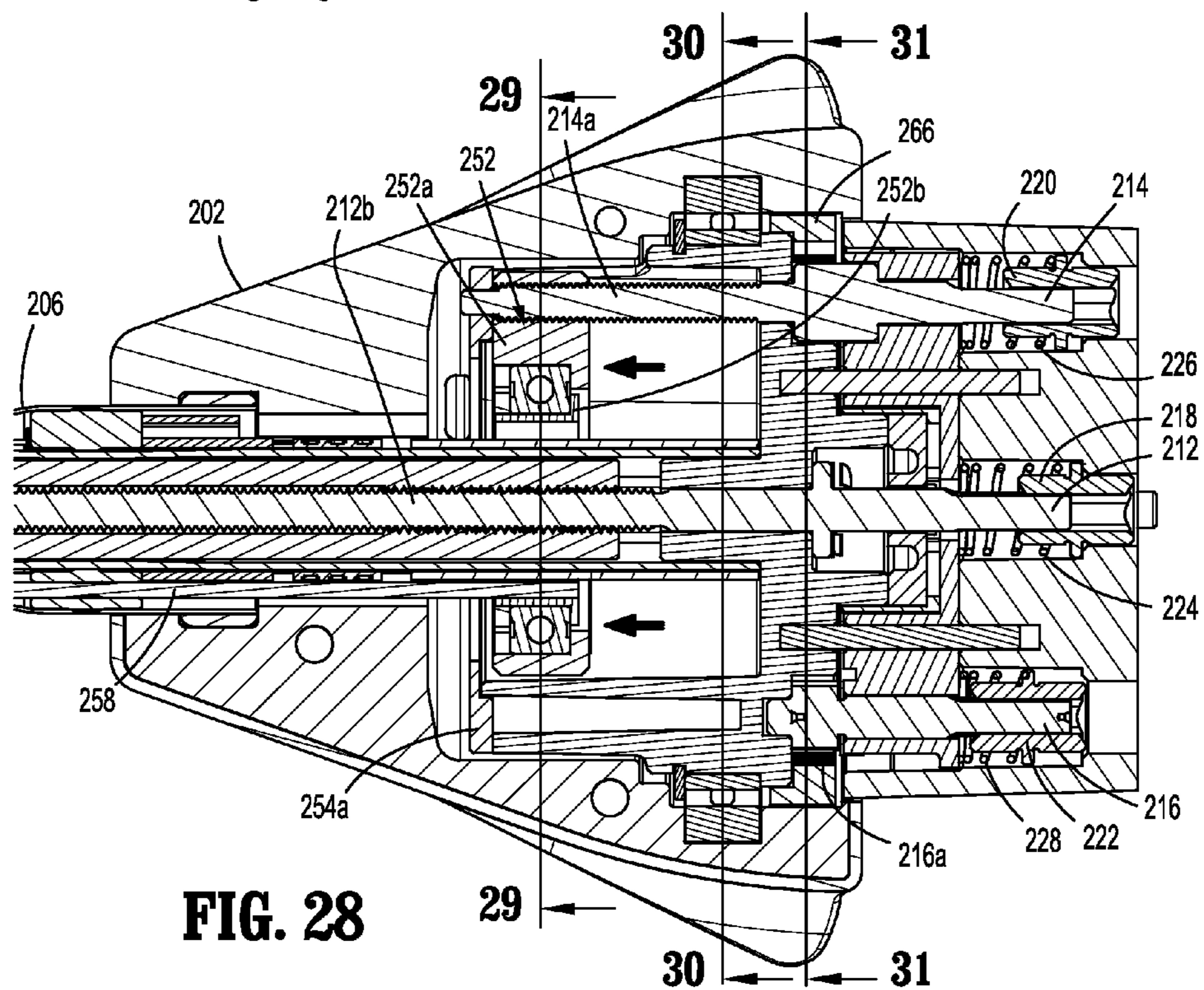
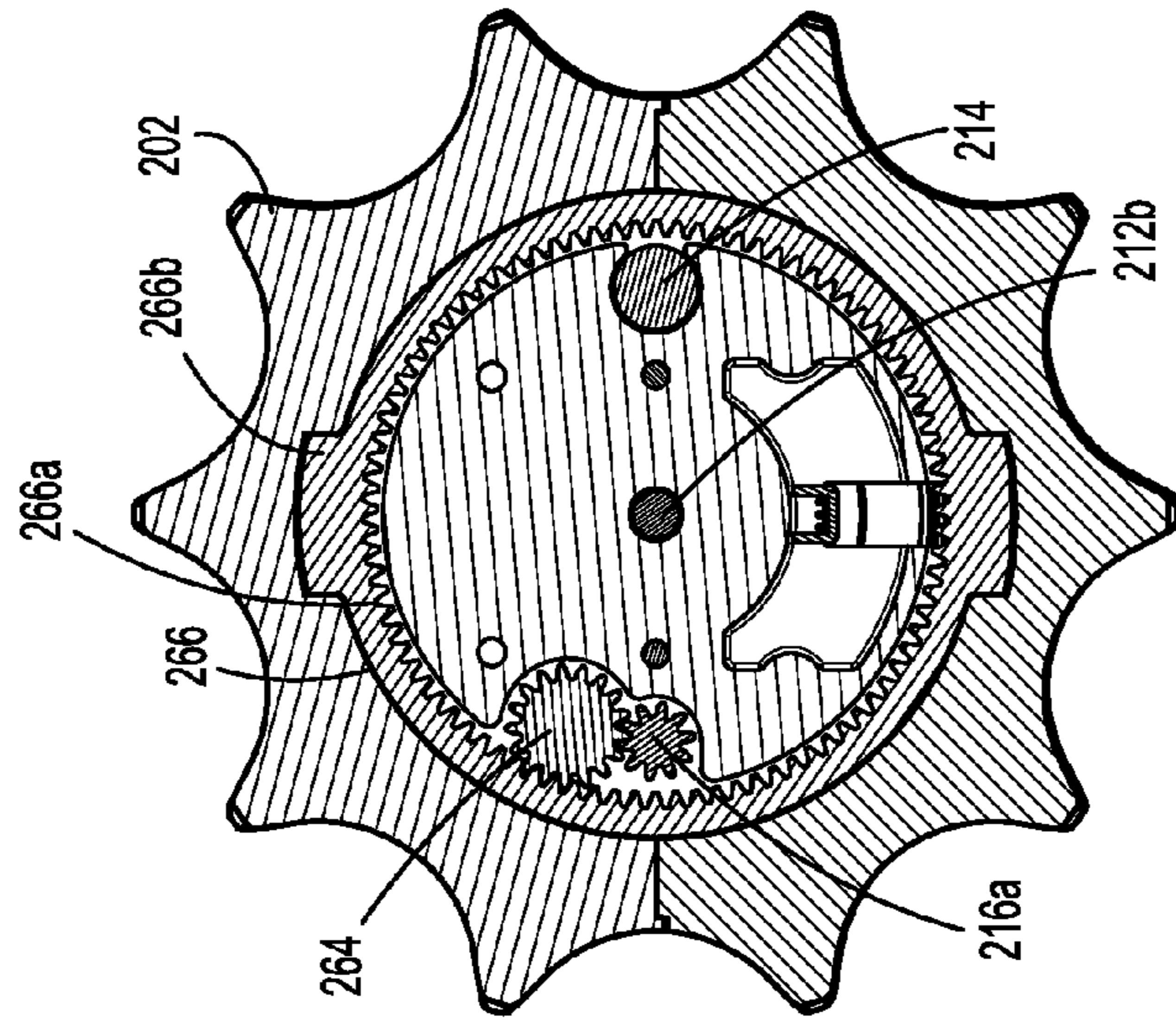
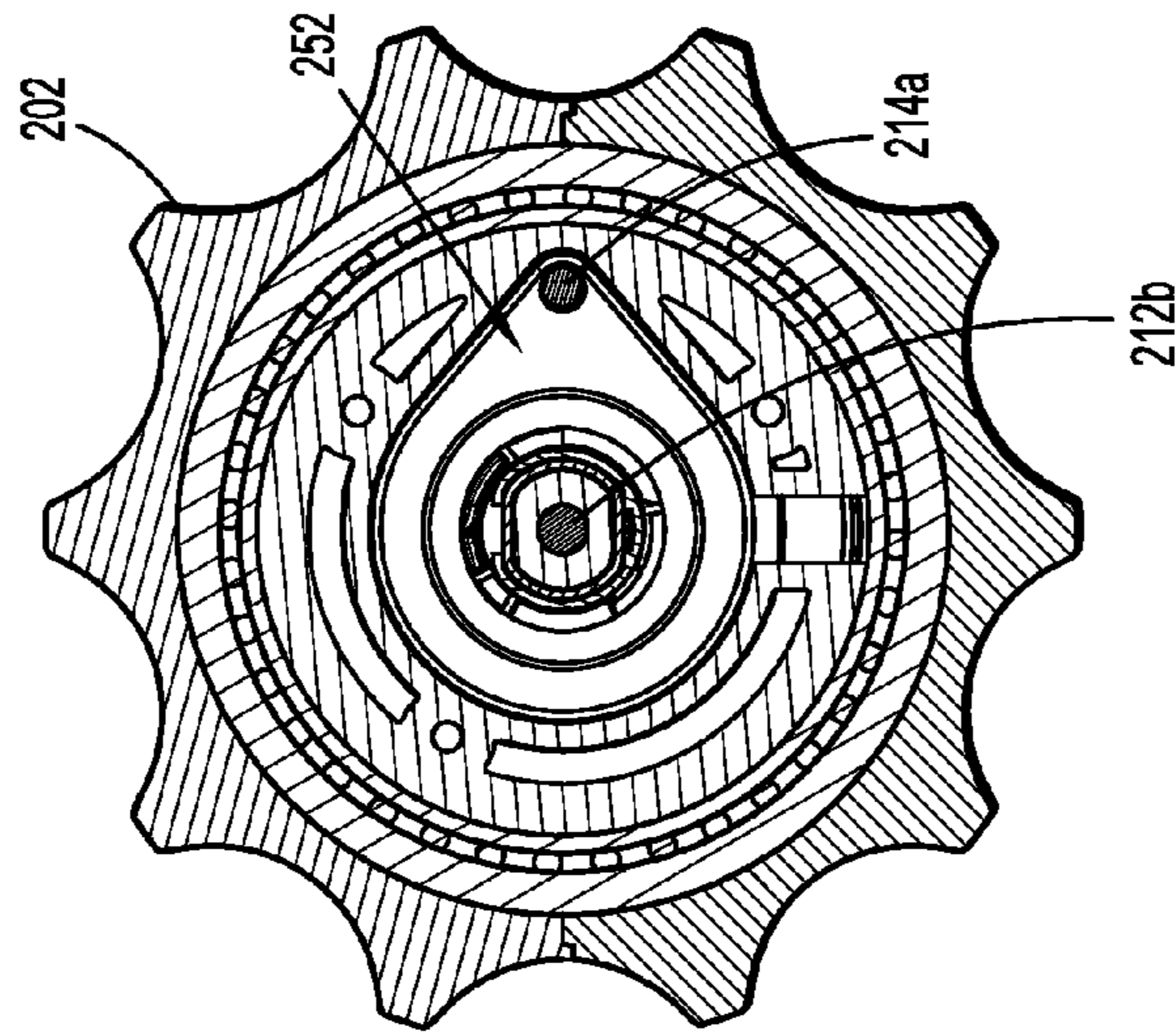


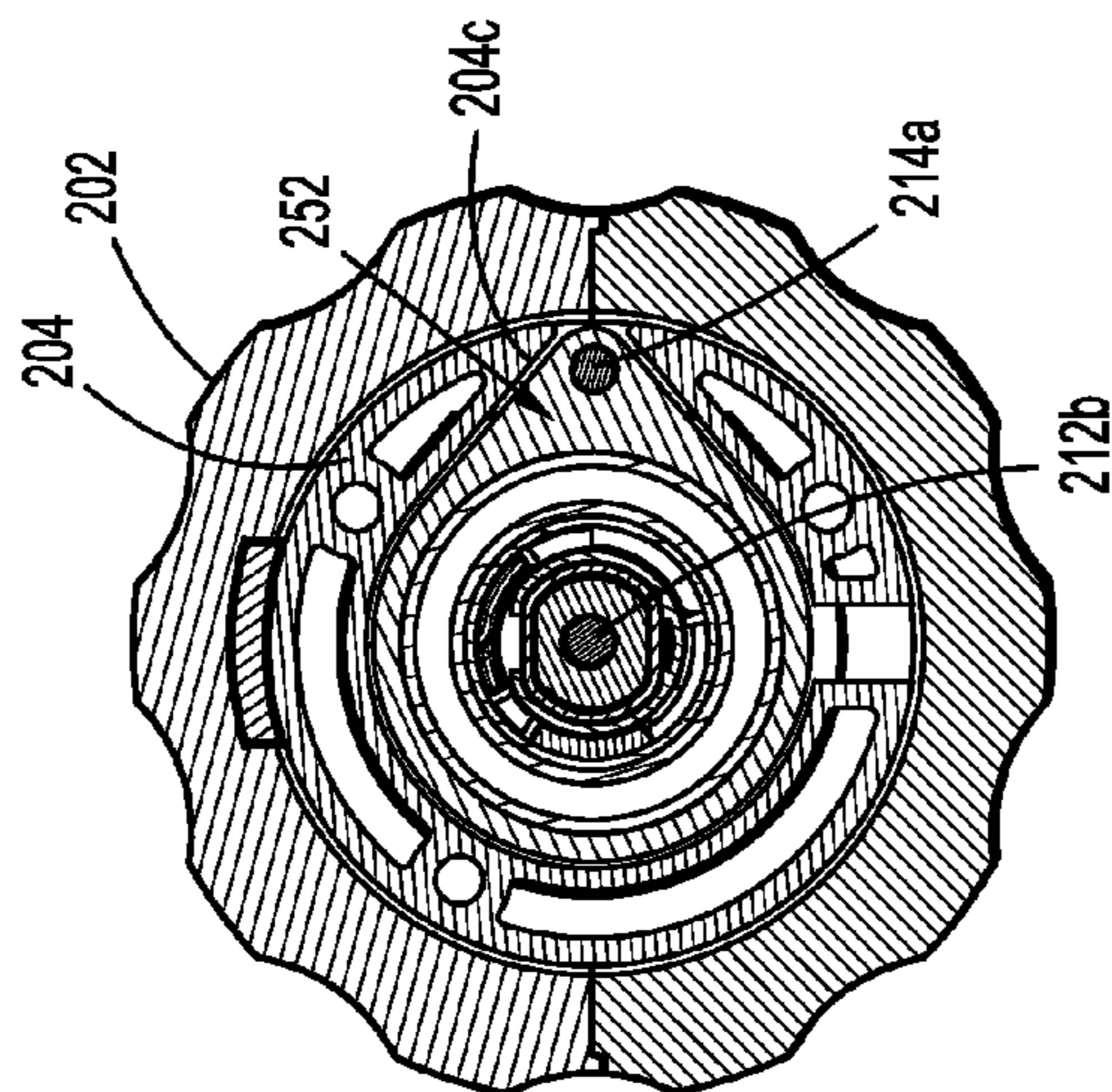
FIG. 28



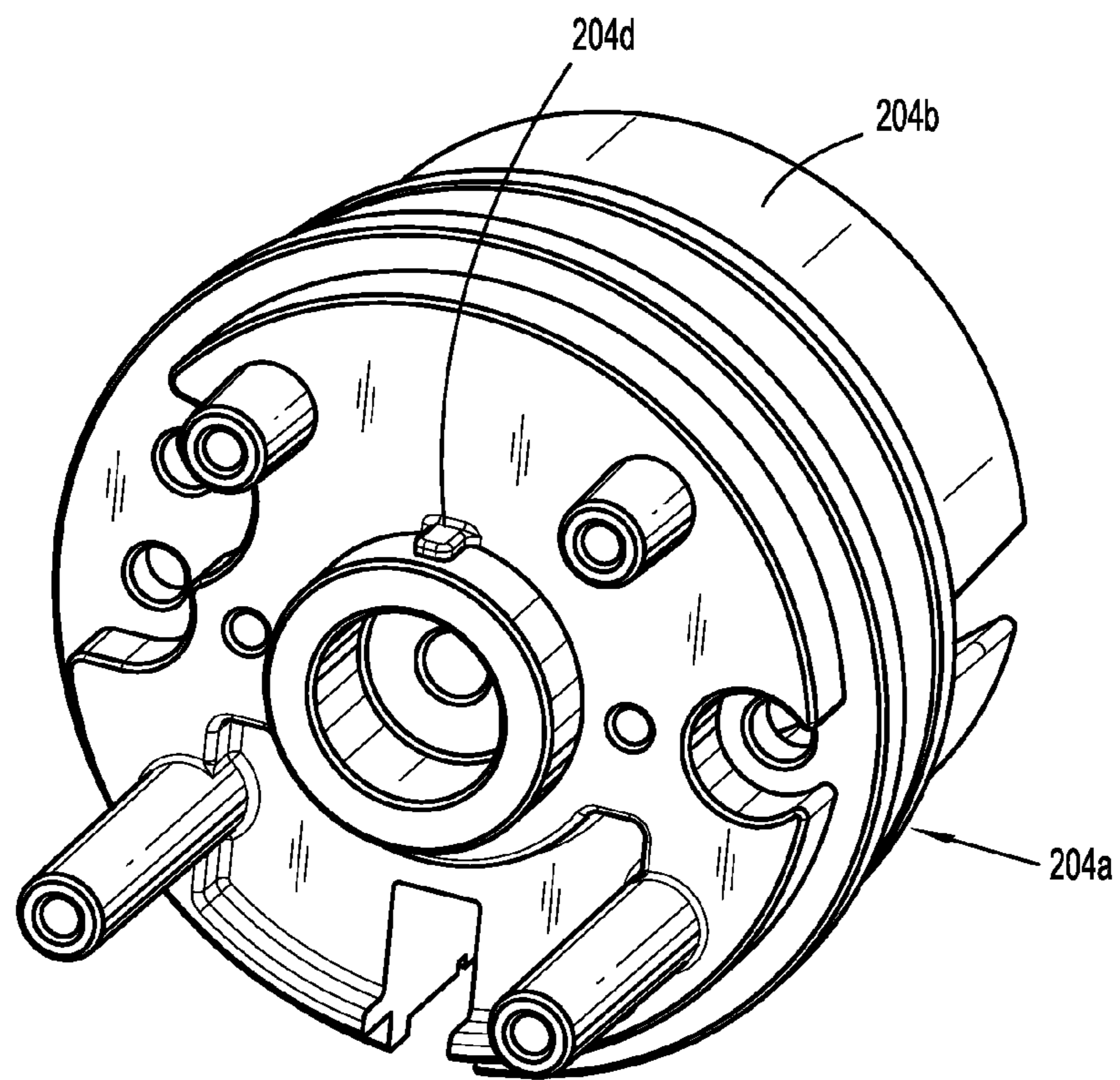
**FIG. 31**



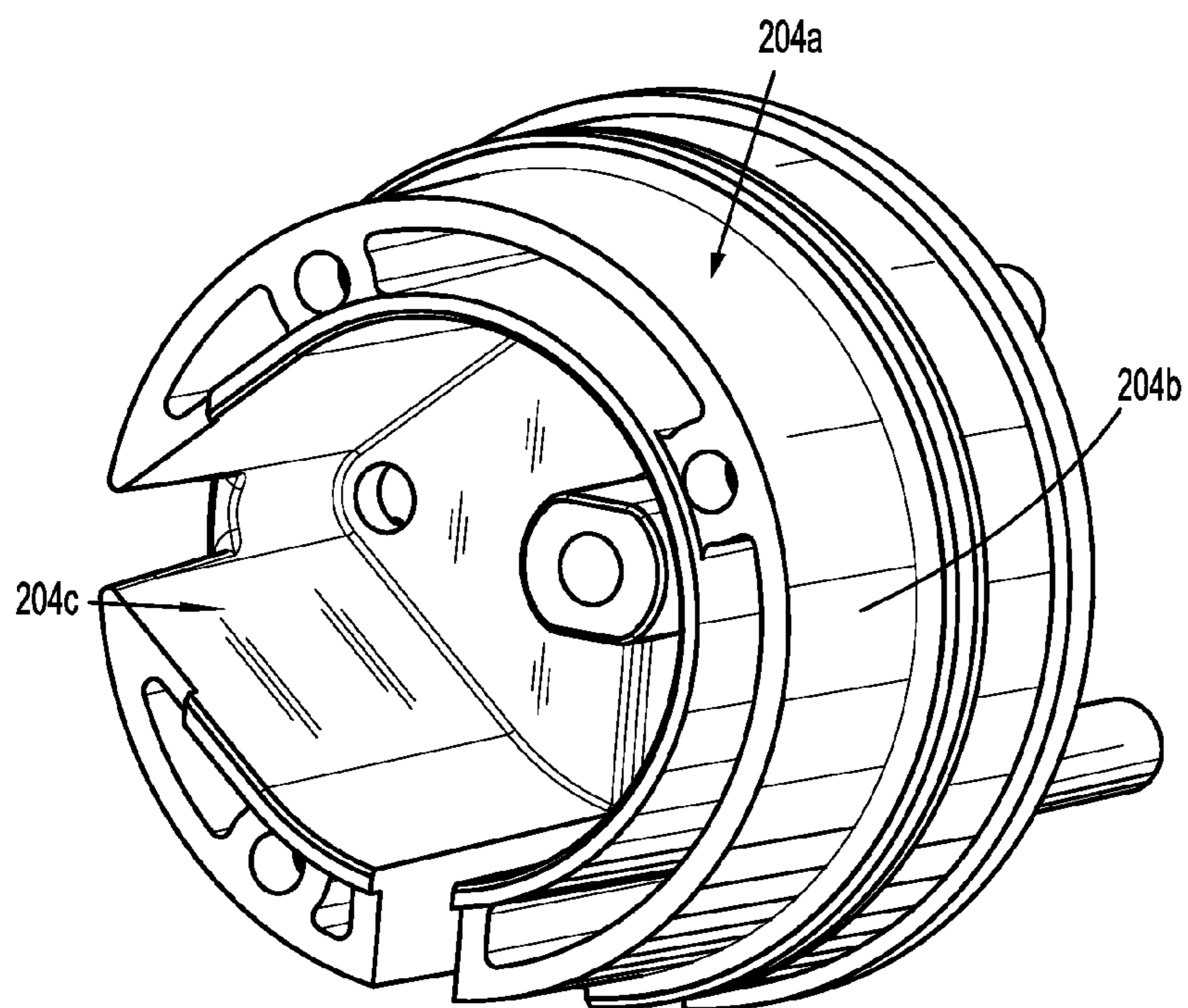
**FIG. 30**



**FIG. 29**

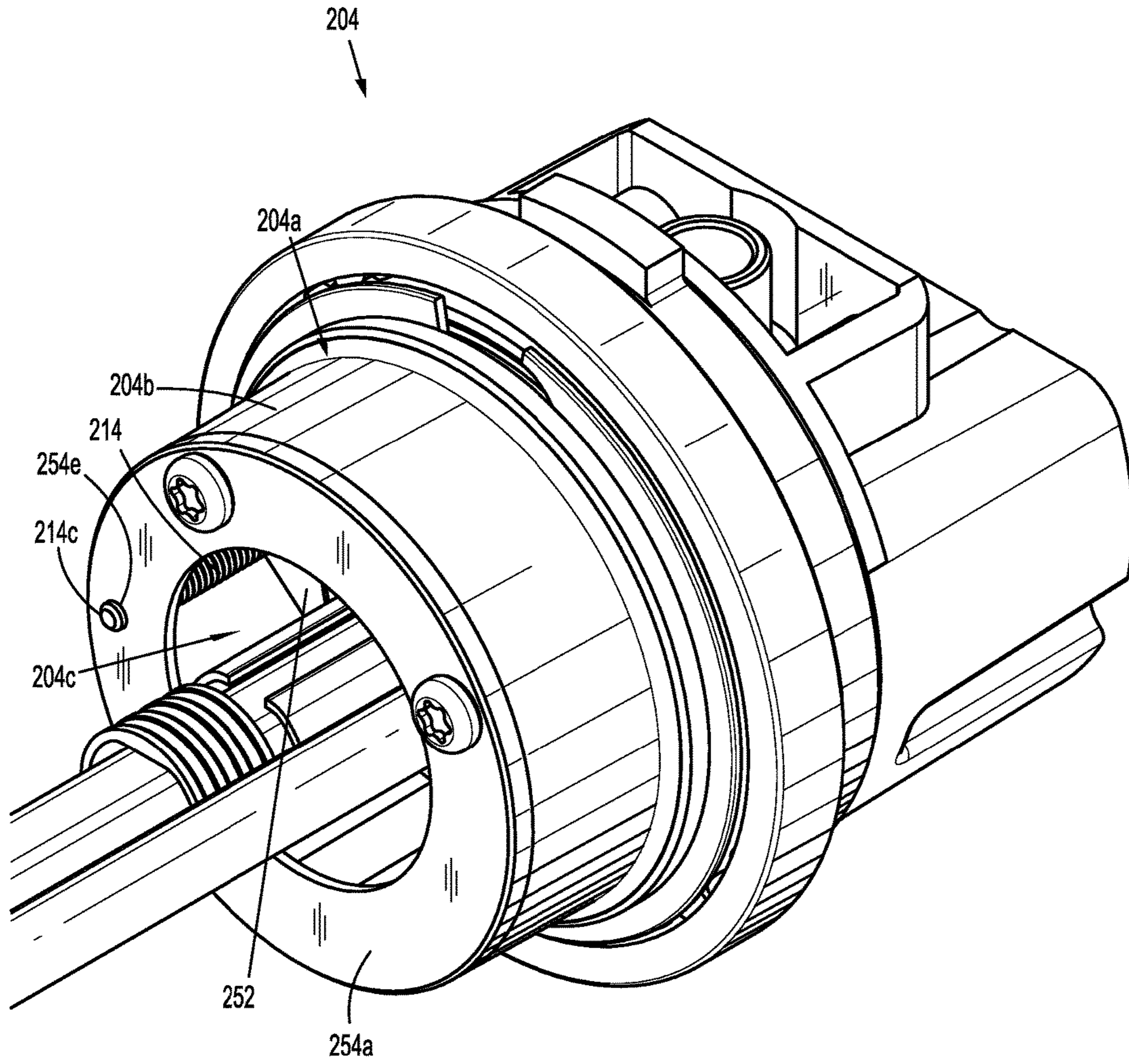


**FIG. 32**

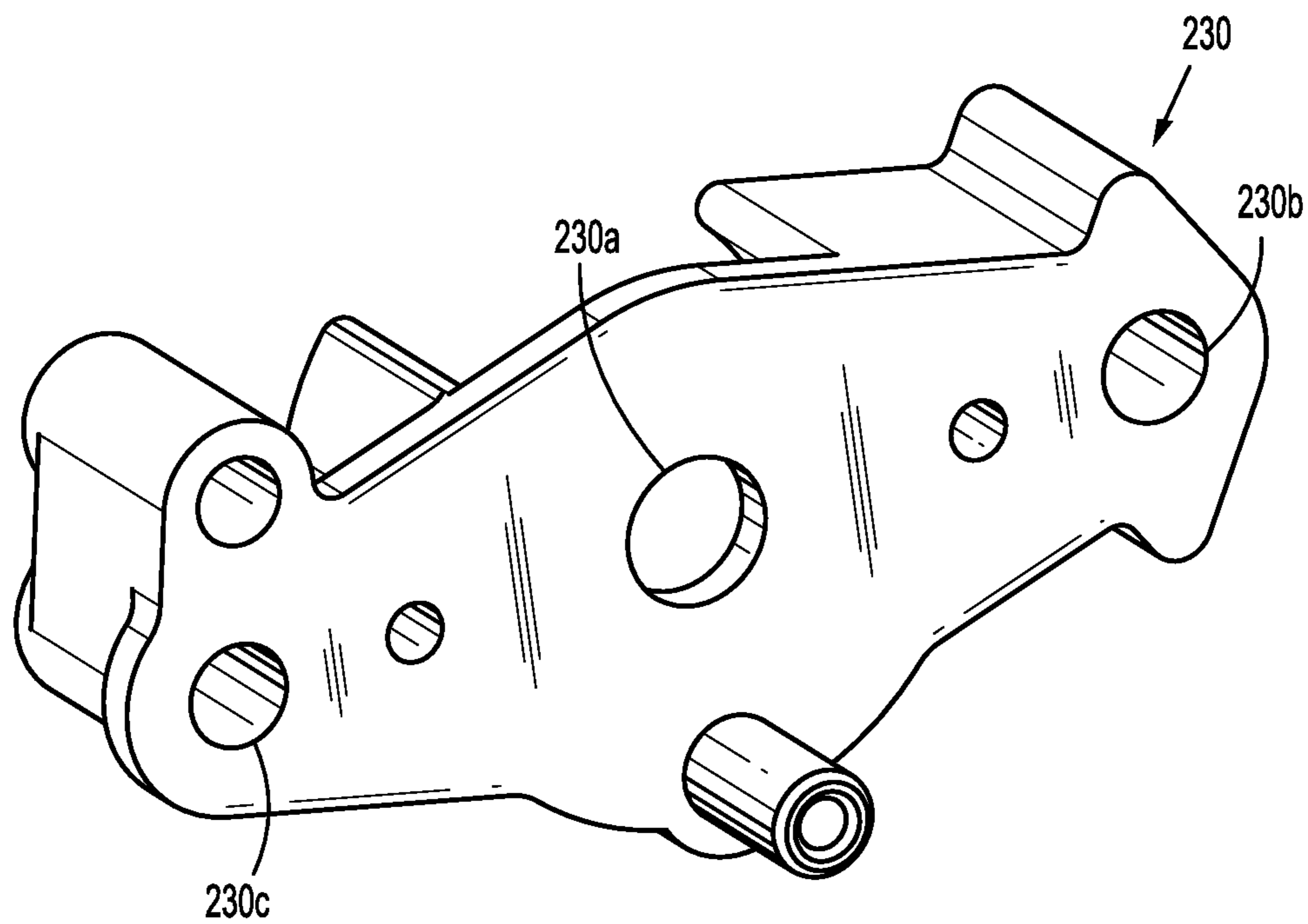


**FIG. 33**

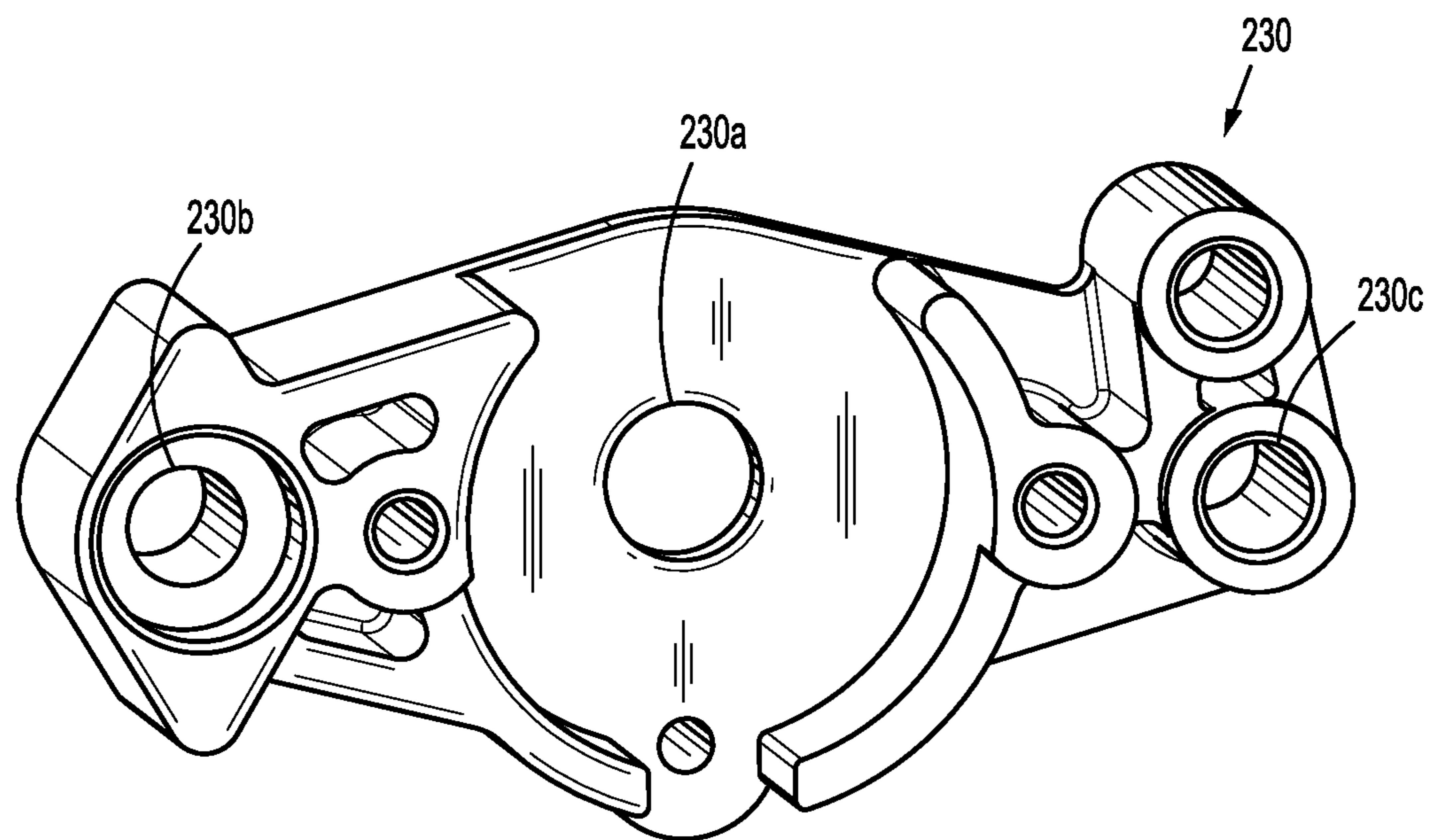




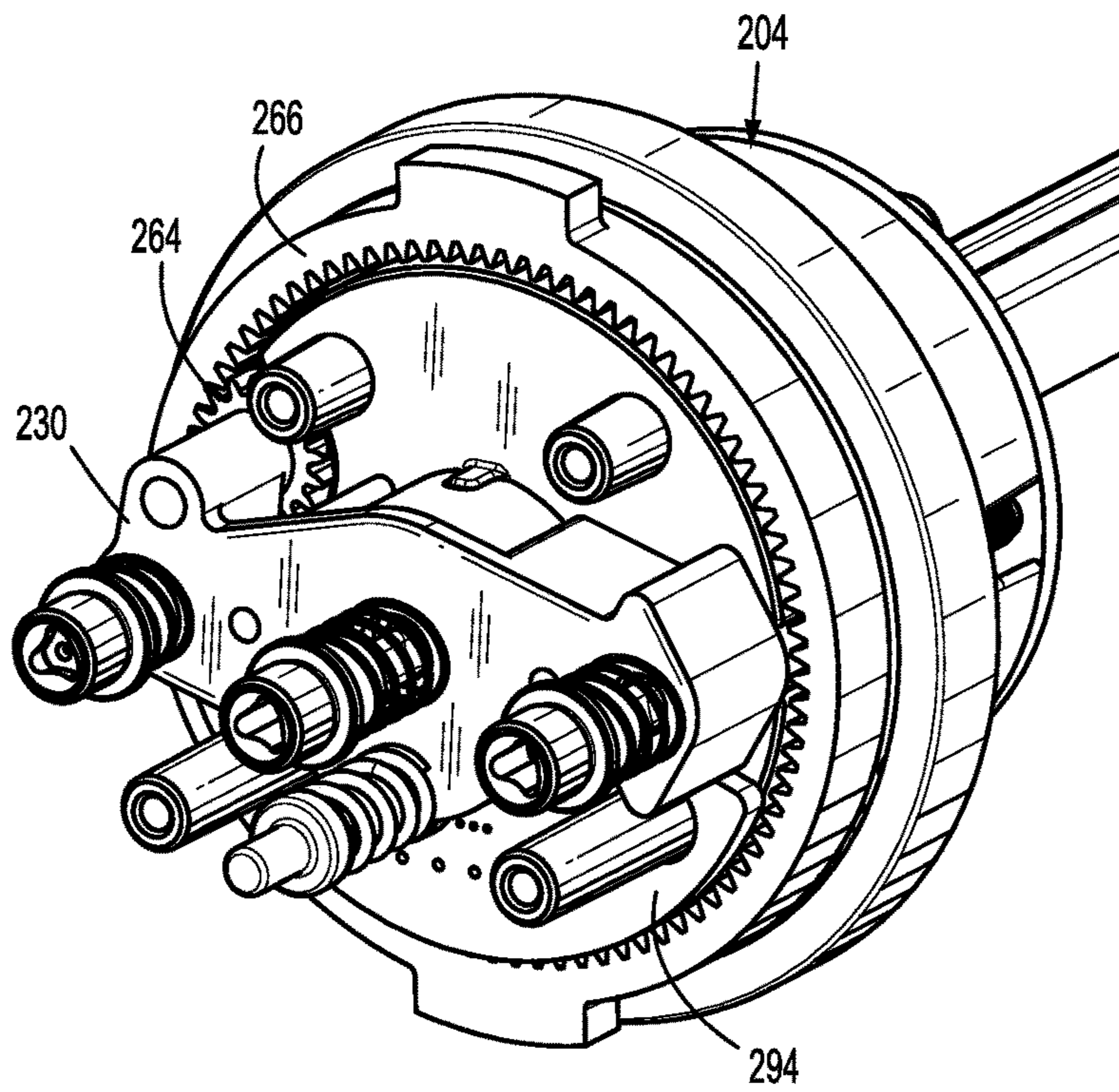
**FIG. 34**



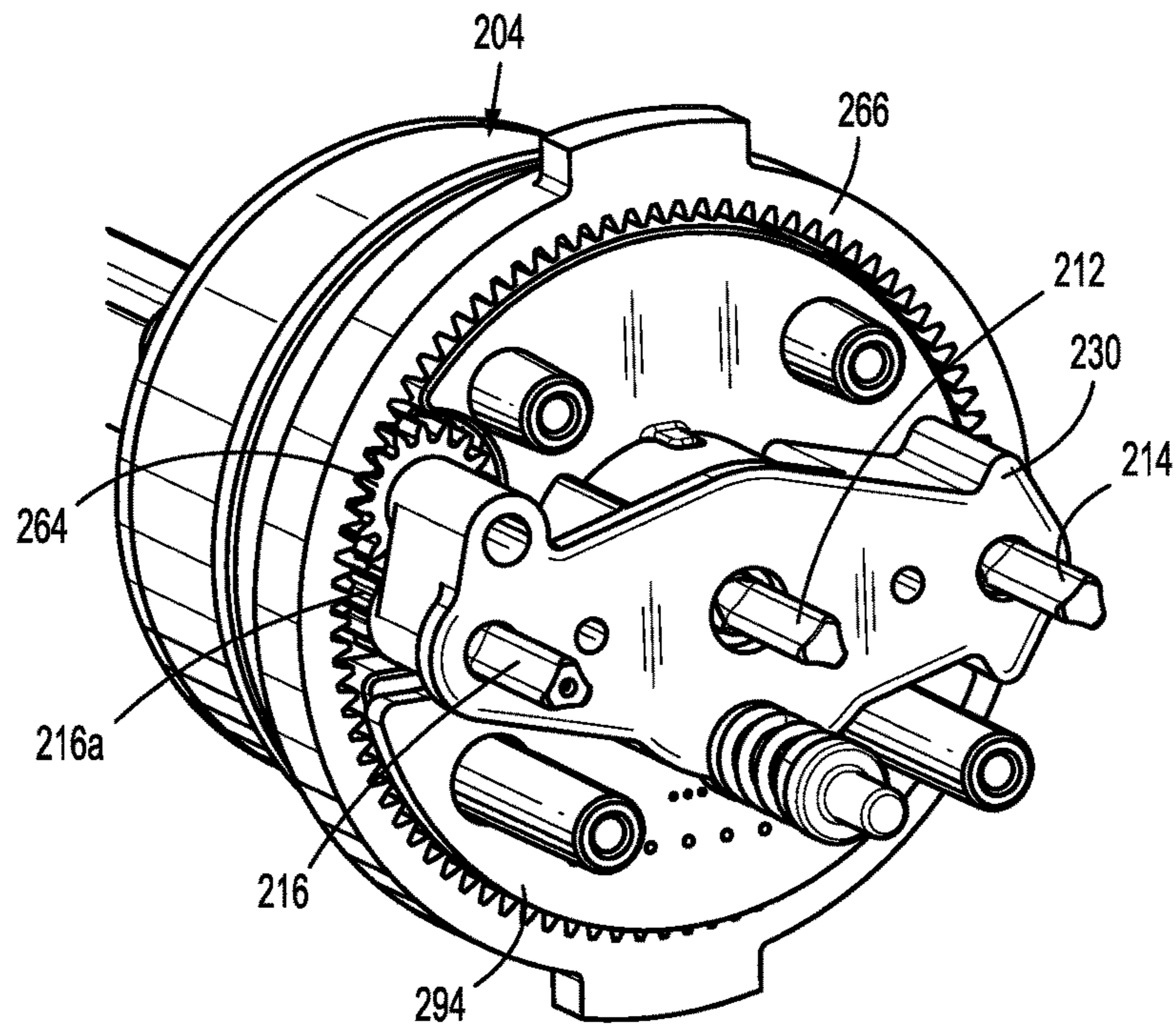
**FIG. 35**



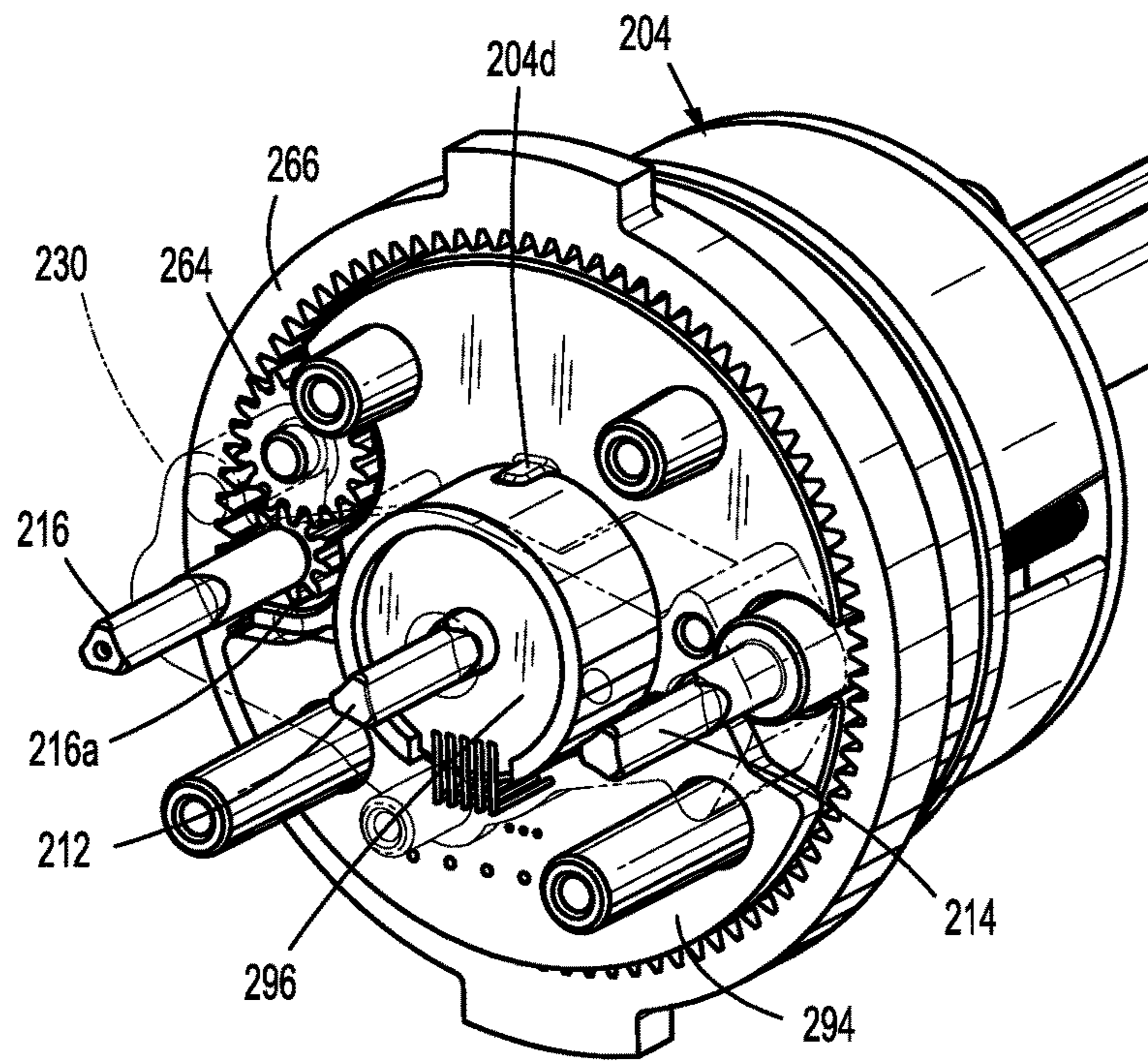
**FIG. 36**



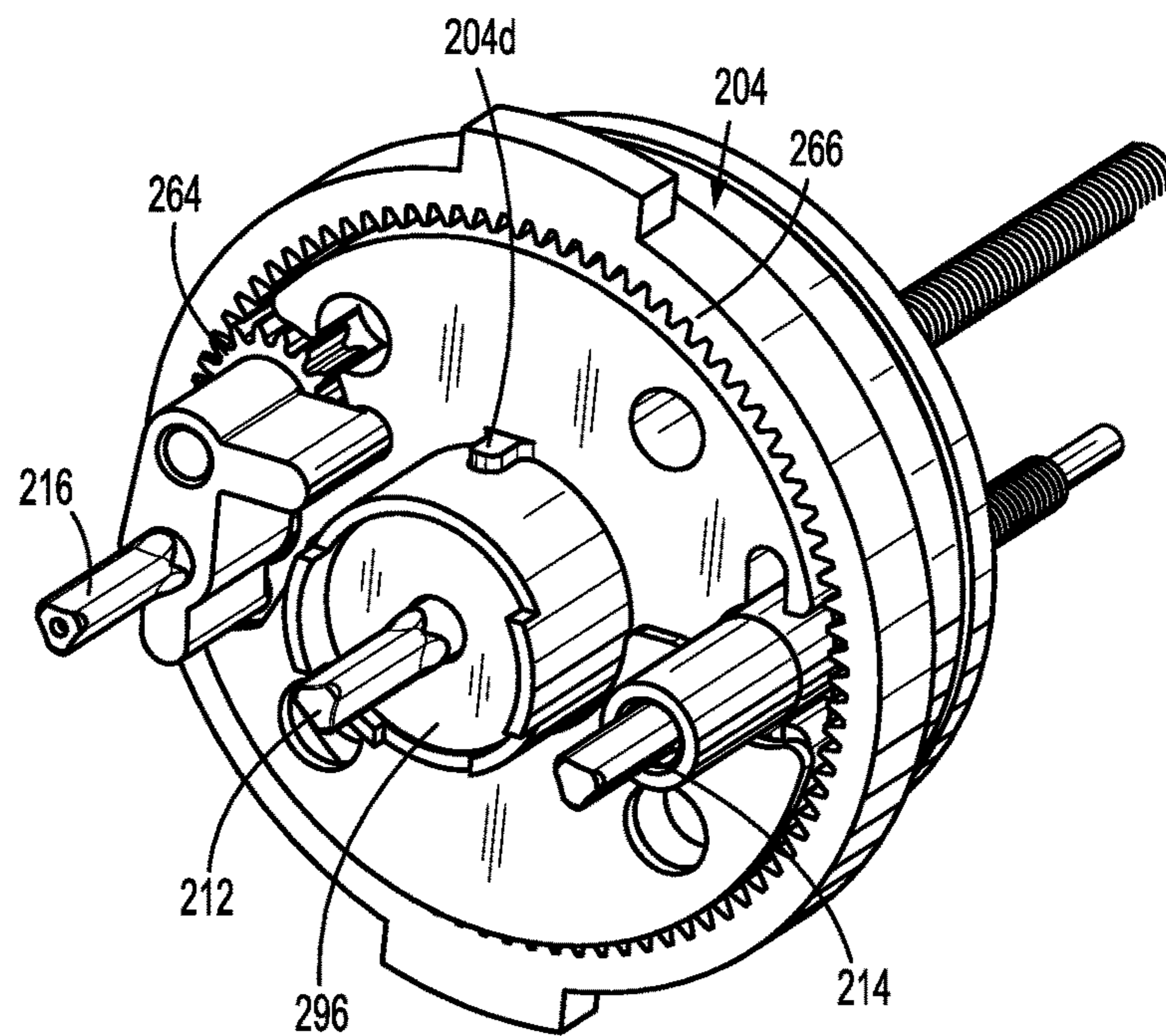
**FIG. 37**



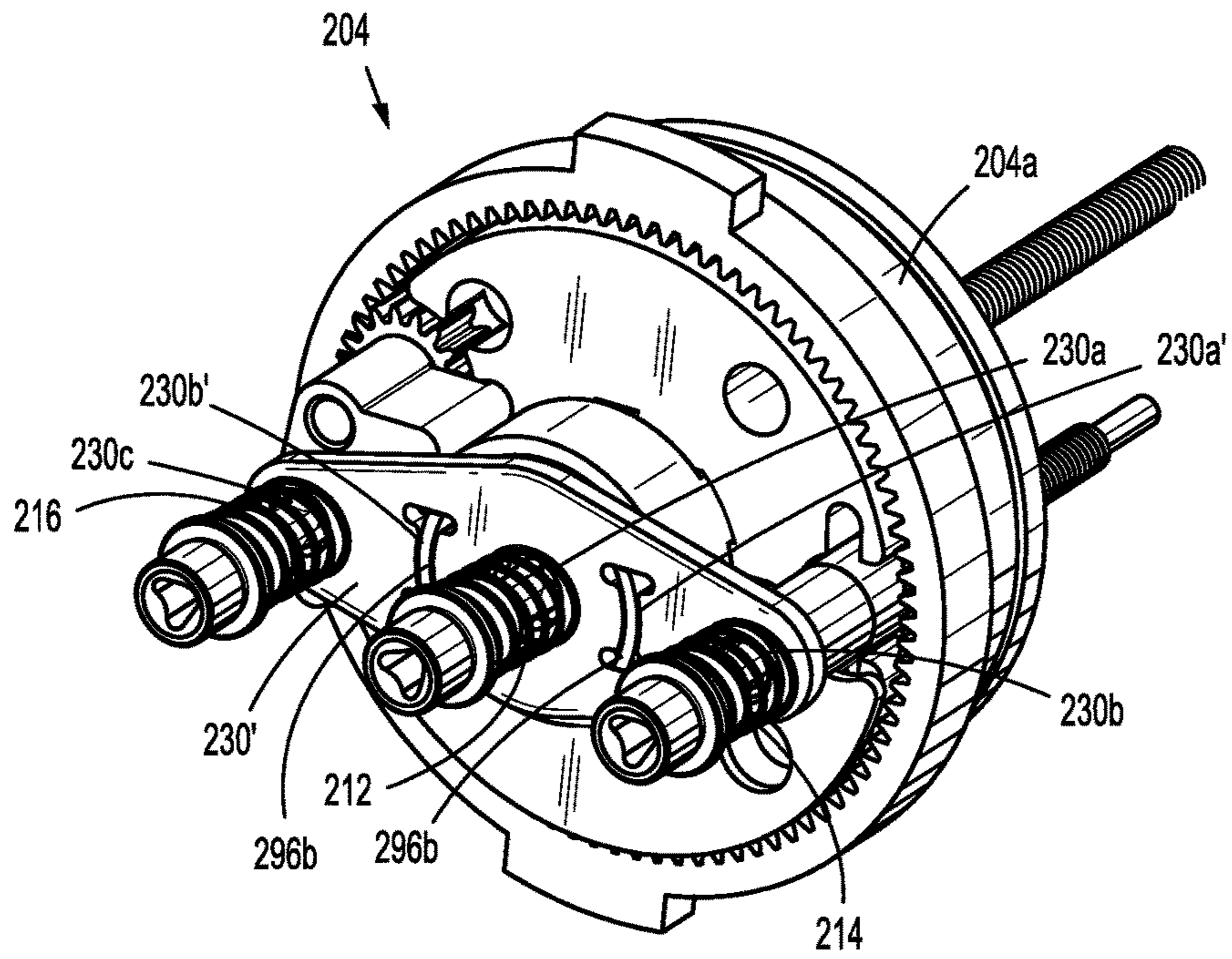
**FIG. 38**



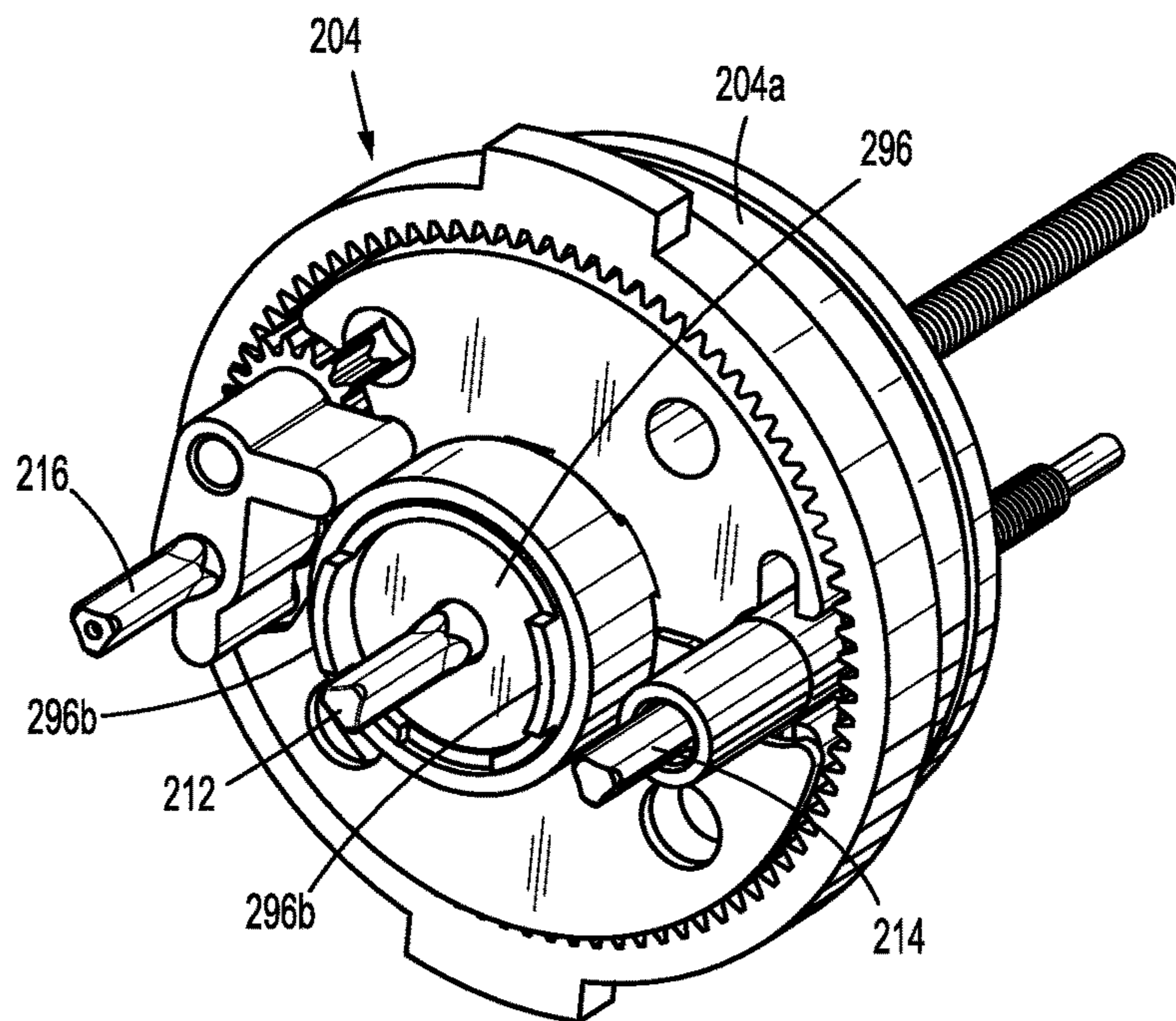
**FIG. 39**



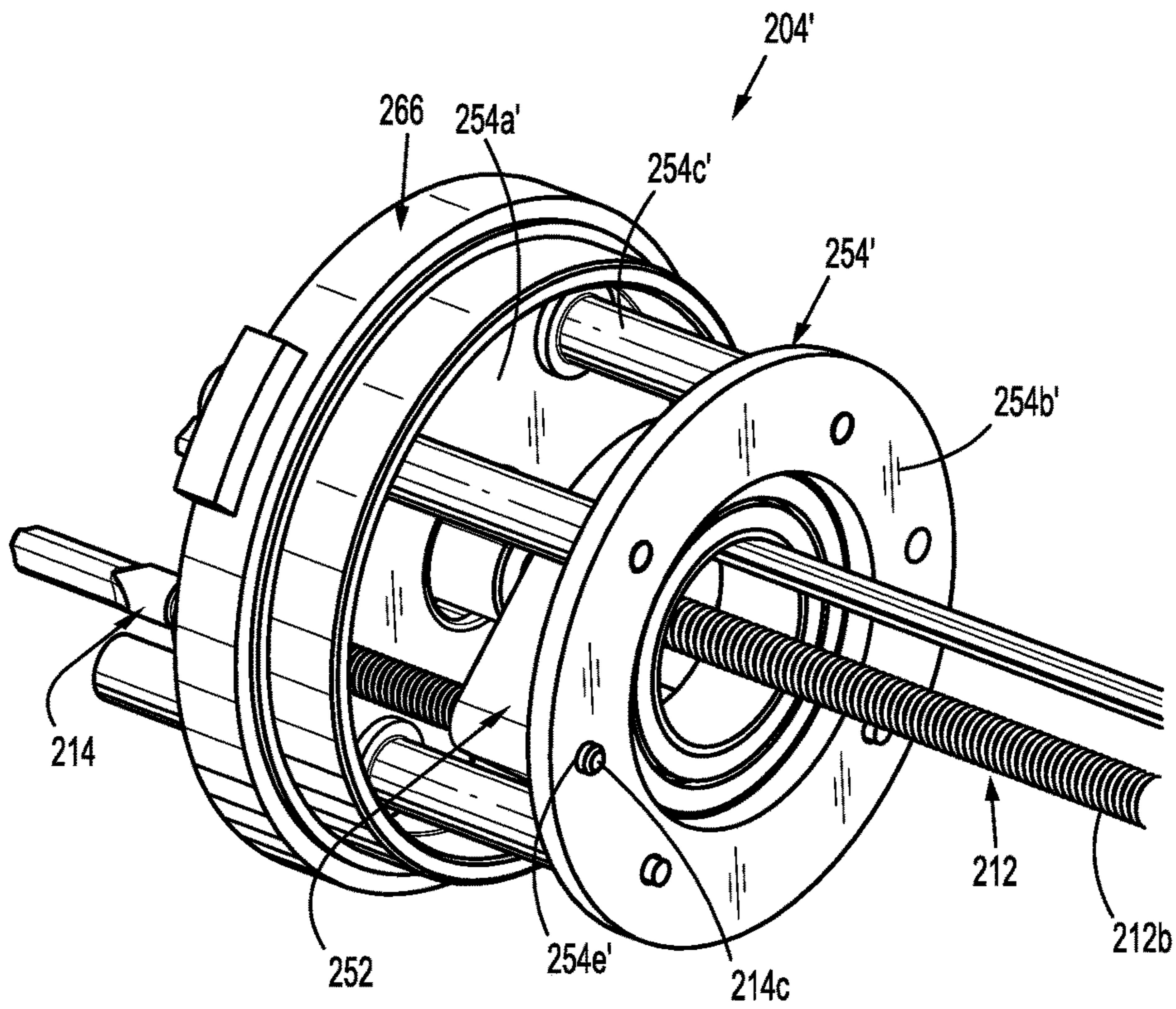
**FIG. 40**



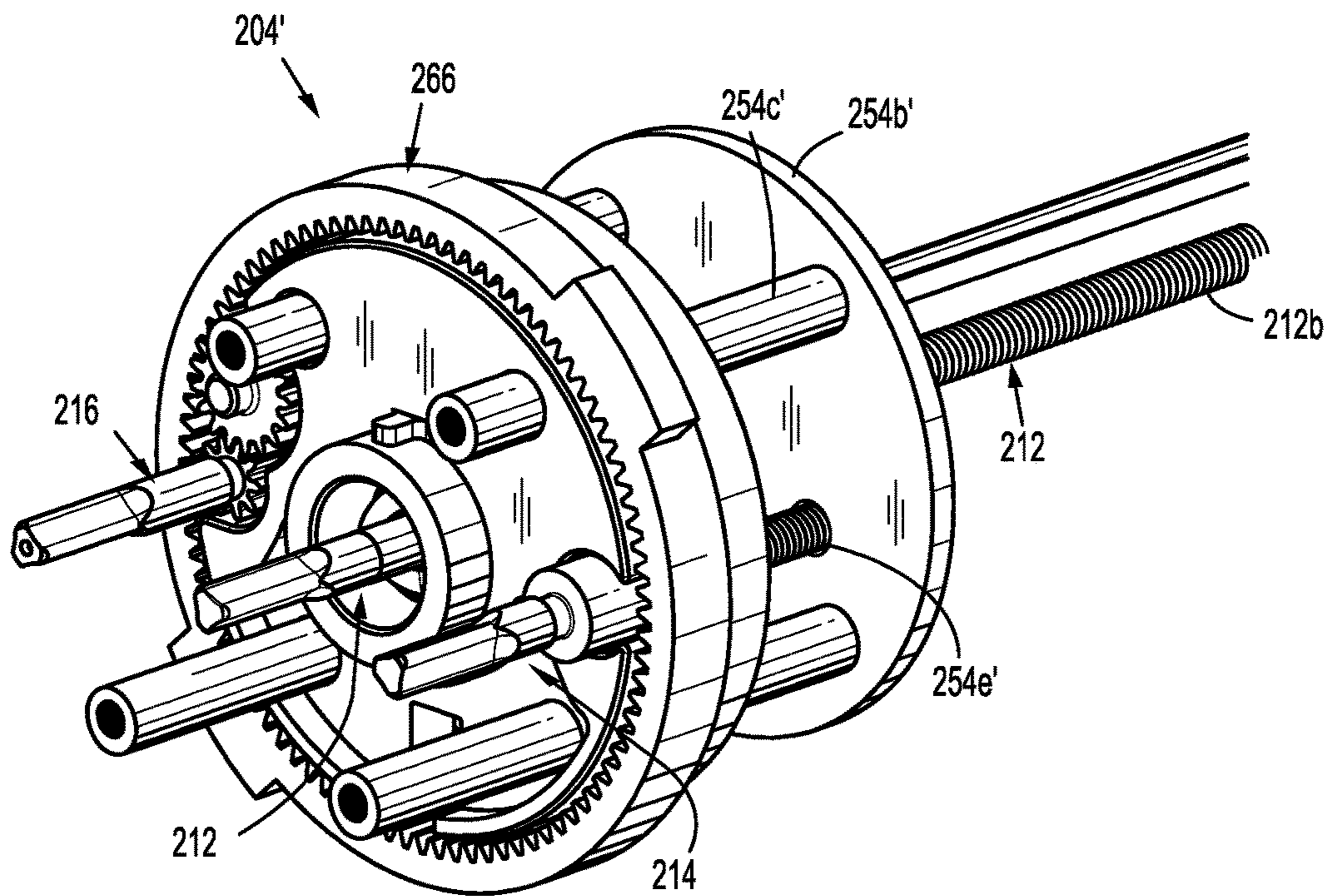
**FIG. 41**



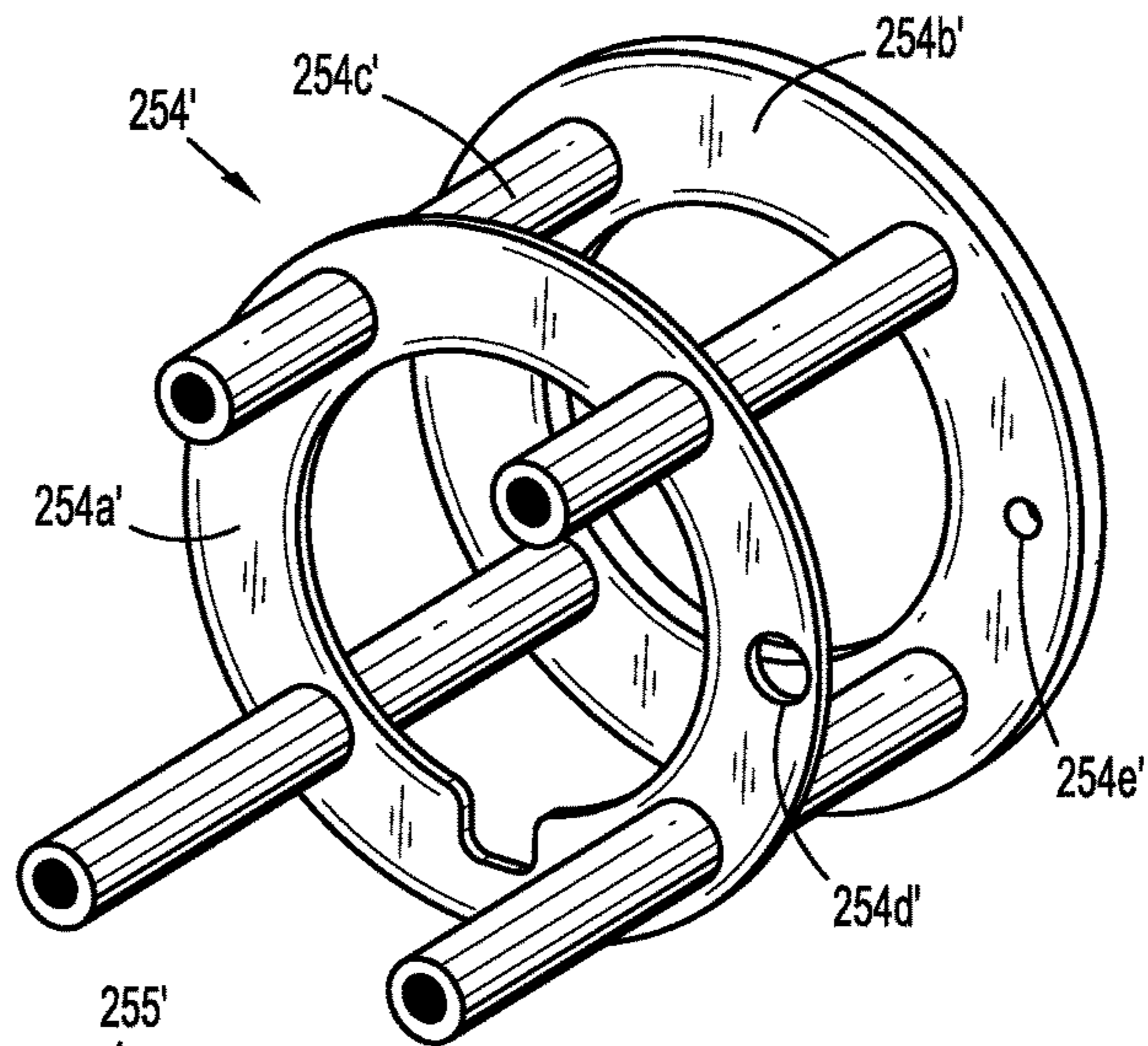
**FIG. 42**



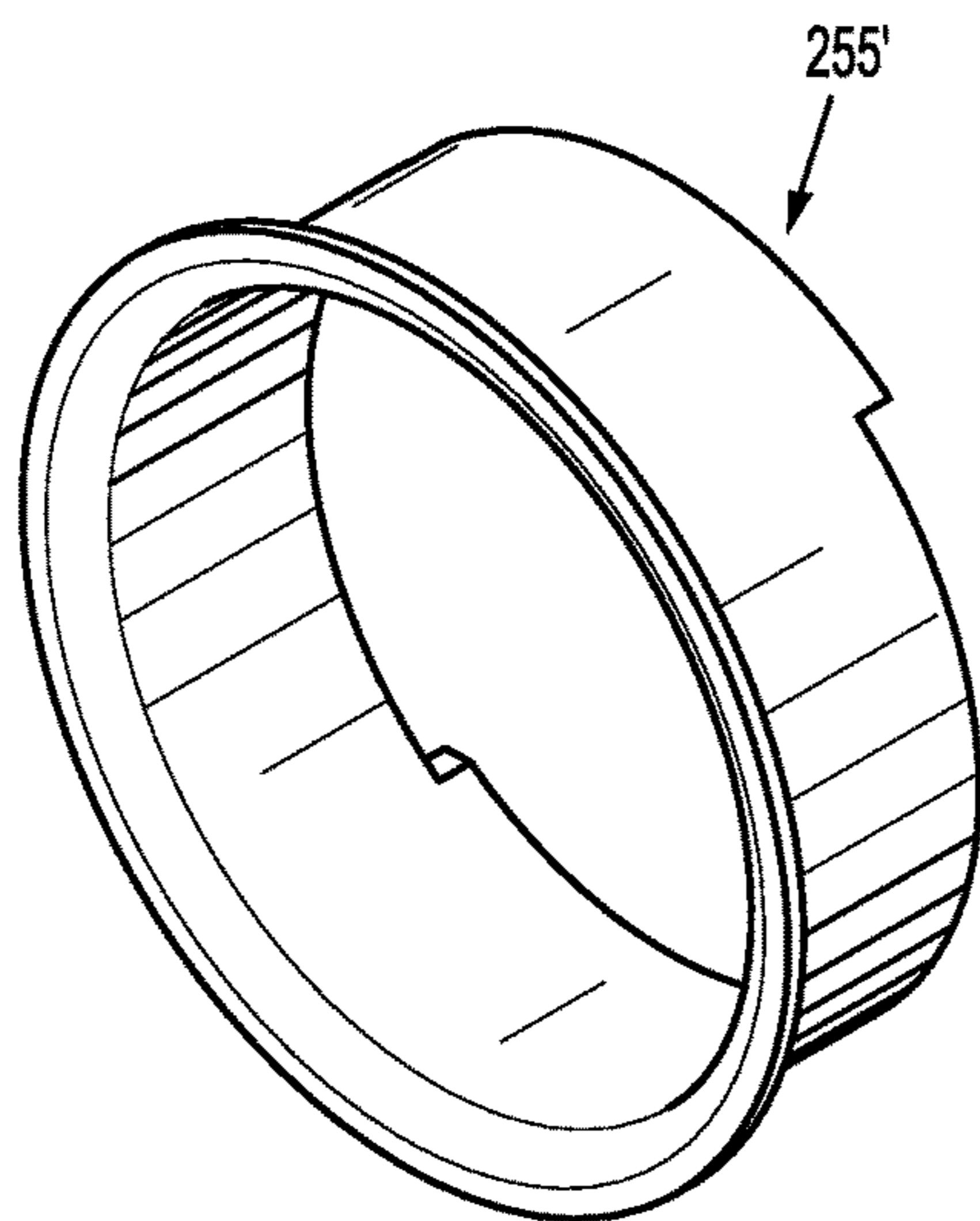
**FIG. 43**



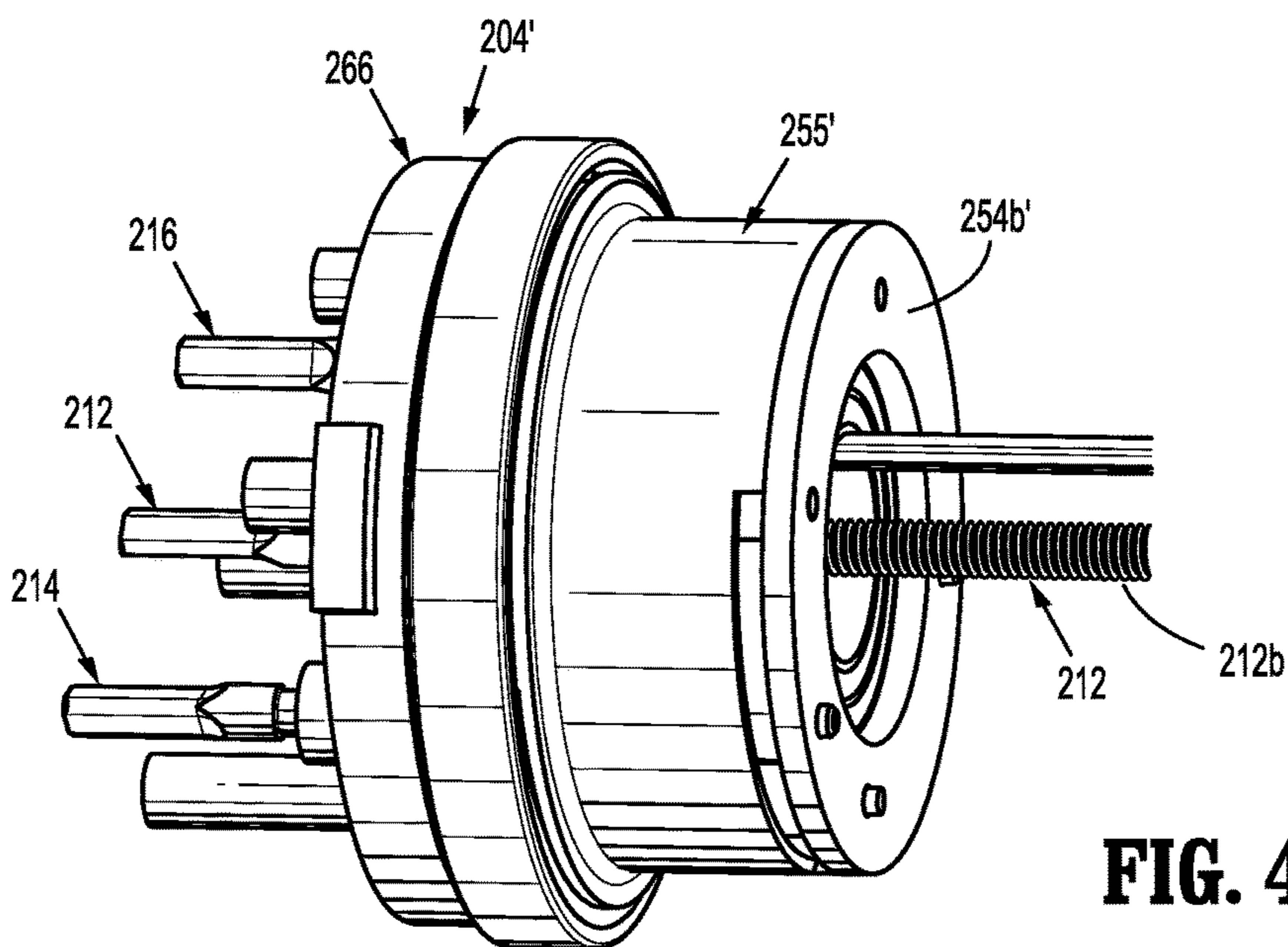
**FIG. 44**



**FIG. 45**



**FIG. 46**



**FIG. 47**

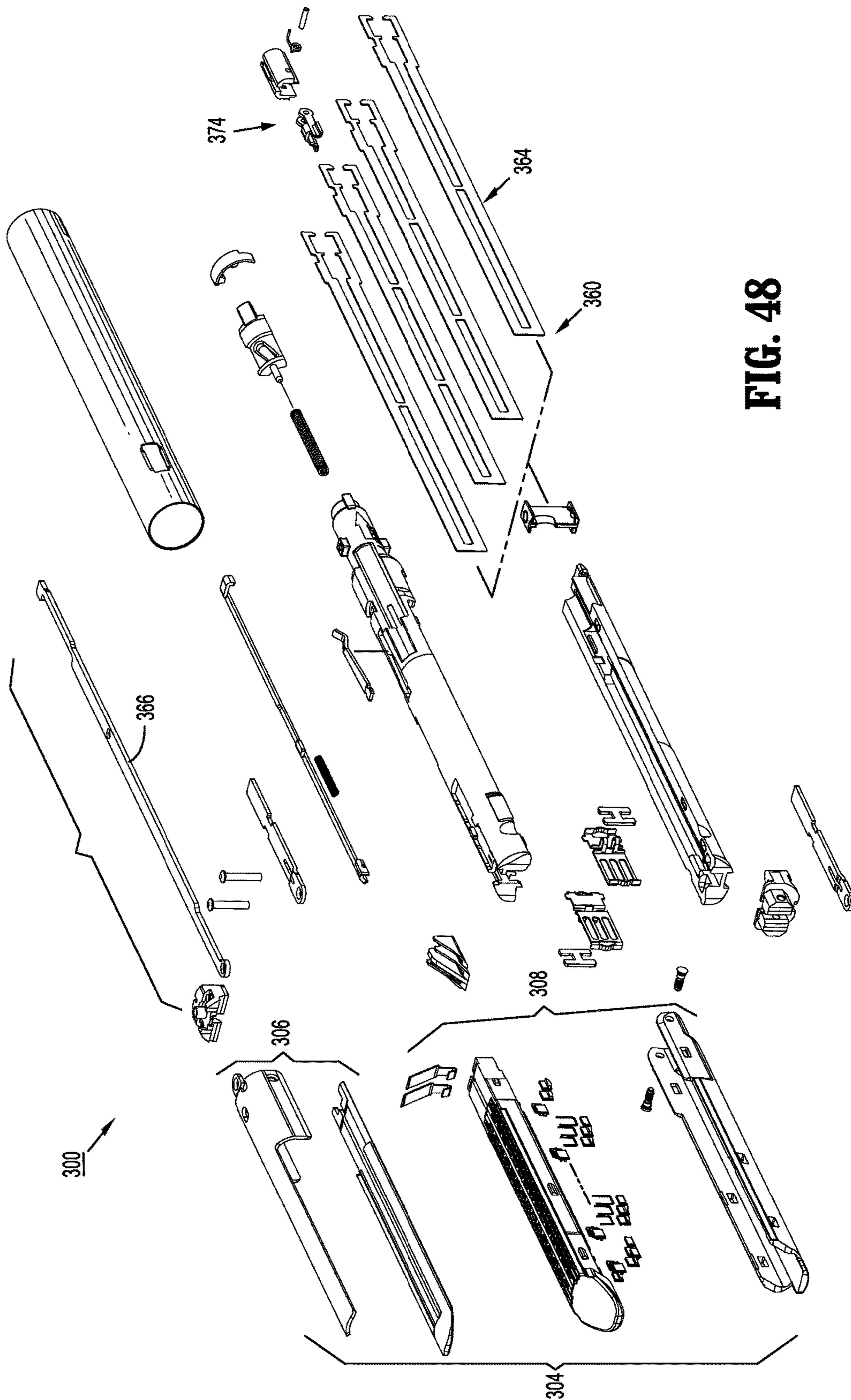


FIG. 48



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**ADAPTER ASSEMBLY FOR  
INTERCONNECTING  
ELECTROMECHANICAL SURGICAL  
DEVICES AND SURGICAL LOADING UNITS,  
AND SURGICAL SYSTEMS THEREOF**

CROSS-REFERENCE TO RELATED  
APPLICATIONS

This application claims the benefit of and priority to U.S. Provisional Patent Application No. 61/913,550, filed Dec. 9, 2013, the entire disclosure of which is incorporated by reference herein.

BACKGROUND

1. Technical Field

The present disclosure relates to adapter assemblies for use in surgical systems. More specifically, the present disclosure relates to adapter assemblies for use with and to electrically and mechanically interconnect electromechanical surgical devices and surgical loading units, and to surgical systems including hand held electromechanical surgical devices and adapter assemblies for connecting surgical loading units to the hand held electromechanical surgical devices.

2. Background of Related Art

A number of surgical device manufacturers have developed product lines with proprietary drive systems for operating and/or manipulating electromechanical surgical devices. In many instances the electromechanical surgical devices include a handle assembly, which is reusable, and disposable loading units and/or single use loading units or the like that are selectively connected to the handle assembly prior to use and then disconnected from the handle assembly following use in order to be disposed of or in some instances sterilized for re-use.

In certain instances, an adapter assembly is used to interconnect an electromechanical surgical device with any one of a number of surgical loading units to establish a mechanical and/or electrical connection therebetween. By using an adapter assembly to interconnect the electromechanical surgical device with the surgical loading units, an overall length of this electromechanical surgical system tends to be relatively greater/longer as compared to an electromechanical surgical system not using an adapter assembly. This increased length of the electromechanical surgical system (including an adapter assembly) tends to move a center of gravity of the electromechanical surgical system (including an adapter assembly) relatively distal of a center of gravity of another electromechanical surgical system (not including an adapter assembly).

With the center of gravity being located at a more distal location of the electromechanical surgical system, a torque exerted on the hand, wrist and arm of the user is increased and thus renders use of the electromechanical surgical system tiresome or cumbersome.

Accordingly, a need exists for an adapter assembly that has a relatively shorter length and that reduces the distal displacement of a center of gravity of the electromechanical surgical system.

SUMMARY

The present disclosure relates to adapter assemblies for use with and to electrically and mechanically interconnect electromechanical surgical devices and surgical loading

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units, and to surgical systems including hand held electromechanical surgical devices and adapter assemblies for connecting surgical loading units to the hand held electromechanical surgical devices.

According to an aspect of the present disclosure, an adapter assembly for selectively interconnecting a surgical loading unit that is configured to perform a function and a surgical device that is configured to actuate the loading unit, is provided. The loading unit may include at least one axially translatable drive member, and the surgical device may include at least one rotatable drive shaft. The adapter assembly includes a housing configured and adapted for connection with the surgical device and to be in operative communication with each rotatable drive shaft of the surgical device; an outer tube having a proximal end supported by the housing and a distal end configured and adapted for connection with the loading unit, wherein the distal end of the outer tube is in operative communication with each of the axially translatable drive member of the loading unit; and the force/rotation transmitting/converting assembly for interconnecting a respective one drive shaft of the surgical device and a respective one axially translatable drive member of the loading unit.

The force/rotation transmitting/converting assembly includes a proximal rotation receiving member that is connectable to a respective rotatable drive shaft of the surgical device; and a distal force transmitting member that is connectable to an axially translatable drive member of the loading unit, the distal force transmitting member being connected to the proximal rotation receiving member in such a manner whereby rotation of the proximal rotation receiving member is converted to axial translation of the distal force transmitting member.

In operation, the force/rotation transmitting/converting assembly converts and transmits a rotation of the first rotatable drive shaft of the surgical device to an axial translation of the first axially translatable drive member of the loading unit.

The force/rotation transmitting/converting assembly may include a first force/rotation transmitting/converting assembly. The proximal rotation receiving member of the first force/rotation transmitting/converting assembly may include a first proximal drive shaft defining a threaded distal end. The distal force transmitting member of the first force/rotation transmitting/converting assembly may include a distal drive member threadably connected to the threaded distal end of the first proximal drive shaft.

The first proximal drive shaft and the distal drive member may be axially aligned with one another and with a rotational axis of the respective rotatable drive shaft of the surgical device.

In use, rotation of the rotatable drive shaft of the surgical device, associated with the first force/rotation transmitting/converting assembly, may result in rotation of the first rotatable drive shaft of the first force/rotation transmitting/converting assembly which may result in axial translation of the distal drive member of the first force/rotation transmitting/converting assembly.

The force/rotation transmitting/converting assembly may include a second force/rotation transmitting/converting assembly. The proximal rotation receiving member of the second force/rotation transmitting/converting assembly may include a second proximal drive shaft defining a threaded distal end. The distal force transmitting member of the second force/rotation transmitting/converting assembly may include a bearing assembly having an outer race threadably

connected to the threaded distal end of the second proximal drive shaft and being non-rotatably disposed within the housing.

The bearing assembly may include an inner race. The distal force transmitting member of the second force/rotation transmitting/converting assembly may include an articulation bar having a proximal end secured to the inner race of the bearing assembly, and a distal end configured to selectively engage a second axially translatable drive member of the loading unit.

At least a portion of the first force/rotation transmitting/converting assembly may extend through the bearing assembly of the second force/rotation transmitting/converting assembly.

The articulation bar may be rotatable about the first force/rotation transmitting/converting assembly.

In use, rotation of the rotatable drive shaft of the surgical device, associated with the second force/rotation transmitting/converting assembly, may result in rotation of the second rotatable drive shaft of the second force/rotation transmitting/converting assembly which results in axial translation of the articulation bar of the second force/rotation transmitting/converting assembly.

The force/rotation transmitting/converting assembly may include a third force/rotation transmitting/converting assembly. The proximal rotation receiving member of the third force/rotation transmitting/converting assembly may include a third proximal drive shaft having a spur gear supported on a distal end thereof. The distal force transmitting member of the third force/rotation transmitting/converting assembly may include a ring gear fixedly supported in the housing and being in gearing connection with the spur gear.

In use, rotation of the rotatable drive shaft of the surgical device, associated with the third force/rotation transmitting/converting assembly, may result in rotation of the third rotatable drive shaft of the third force/rotation transmitting/converting assembly which results in rotation of the ring gear of the third force/rotation transmitting/converting assembly.

The adapter assembly may further include an electrical assembly supported within at least one of the housing and the outer tube. The electrical assembly may include a circuit board; and contact pins electrically connected to the circuit board and being configured and adapted to selectively electrically connect to a complementary electrical plug of the surgical device; a strain gauge supported on and electrically connected to the circuit board, wherein the first rotatable proximal drive shaft extends through the strain gauge; and a slip ring disposed about the distal drive member of the first force/rotation transmitting/converting assembly. The slip ring may be in electrical connection with the circuit board, and wherein the slip ring includes electrical contact supported therein for maintaining electrical contact with electrical components within the adapter assembly.

The first proximal drive shaft, the second proximal drive shaft and the third proximal drive shaft may be arranged in a common plane with one another.

According to another aspect of the present disclosure, an electromechanical surgical system is provided that is configured for selective connection with a surgical loading unit in order to actuate the loading unit to perform functions. The loading unit may include at least one axially translatable drive member. The surgical system includes a handle-held electromechanical surgical device including a housing; and at least one rotatable drive shaft supported in the projecting from the housing.

The surgical system further includes an adapter assembly selectively connectable between the housing of the surgical device and the loading unit. The adapter assembly includes a housing configured and adapted for connection with the surgical device and to be in operative communication with each rotatable drive shaft of the surgical device; an outer tube having a proximal end supported by the housing and a distal end configured and adapted for connection with the loading unit, wherein the distal end of the outer tube is in operative communication with each of the axially translatable drive members of the loading unit; and the force/rotation transmitting/converting assemblies for interconnecting a respective drive shafts of the surgical device and the respective axially translatable drive member of the loading unit.

The force/rotation transmitting/converting assembly includes a proximal rotation receiving member that is connectable to a respective rotatable drive shaft of the surgical device; and a distal force transmitting member that is connectable to an axially translatable drive member of the loading unit, the distal force transmitting member being connected to the proximal rotation receiving member in such a manner whereby rotation of the proximal rotation receiving member is converted to axial translation of the distal force transmitting member.

The force/rotation transmitting/converting assembly converts and transmits a rotation of the first rotatable drive shaft of the surgical device to an axial translation of the first axially translatable drive member of the loading unit.

The force/rotation transmitting/converting assembly of the adapter assembly may include a first force/rotation transmitting/converting assembly. The proximal rotation receiving member of the first force/rotation transmitting/converting assembly may include a first proximal drive shaft defining a threaded distal end. The distal force transmitting member of the first force/rotation transmitting/converting assembly may include a distal drive member threadably connected to the threaded distal end of the first proximal drive shaft.

The first proximal drive shaft and the distal drive member of the adapter assembly may be axially aligned with one another and with a rotational axis of the respective rotatable drive shaft of the surgical device.

In use, rotation of the rotatable drive shaft of the surgical device, associated with the first force/rotation transmitting/converting assembly, may result in rotation of the first rotatable drive shaft of the first force/rotation transmitting/converting assembly which results in axial translation of the distal drive member of the first force/rotation transmitting/converting assembly of the adapter assembly.

The force/rotation transmitting/converting assembly of the adapter assembly may include a second force/rotation transmitting/converting assembly. The proximal rotation receiving member of the second force/rotation transmitting/converting assembly may include a second proximal drive shaft defining a threaded distal end. The distal force transmitting member of the second force/rotation transmitting/converting assembly may include a bearing assembly having an outer race threadably connected to the threaded distal end of the second proximal drive shaft and being non-rotatably disposed within the housing.

The bearing assembly of the adapter assembly may include an inner race, and wherein the distal force transmitting member of the second force/rotation transmitting/converting assembly of the adapter assembly may include an articulation bar having a proximal end secured to the inner

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race of the bearing assembly, and a distal end configured to selectively engage a second axially translatable drive member of the loading unit.

At least a portion of the first force/rotation transmitting/converting assembly of the adapter assembly may extend through the bearing assembly of the second force/rotation transmitting/converting assembly of the adapter assembly.

The articulation bar of the adapter assembly may be rotatable about the first force/rotation transmitting/converting assembly.

In use, rotation of the rotatable drive shaft of the surgical device, associated with the second force/rotation transmitting/converting assembly of the adapter assembly, may result in rotation of the second rotatable drive shaft of the second force/rotation transmitting/converting assembly which may result in axial translation of the articulation bar of the second force/rotation transmitting/converting assembly.

The force/rotation transmitting/converting assembly of the adapter assembly may include a third force/rotation transmitting/converting assembly. The proximal rotation receiving member of the third force/rotation transmitting/converting assembly may include a third proximal drive shaft having a spur gear supported on a distal end thereof. The distal force transmitting member of the third force/rotation transmitting/converting assembly may include a ring gear fixedly supported in the housing and being in gearing connection with the spur gear.

In use, rotation of the rotatable drive shaft of the surgical device, associated with the third force/rotation transmitting/converting assembly, may result in rotation of the third rotatable drive shaft of the third force/rotation transmitting/converting assembly of the adapter assembly which may result in rotation of the ring gear of the third force/rotation transmitting/converting assembly.

The adapter assembly may further include an electrical assembly supported within at least one of the housing and the outer tube thereof. The electrical assembly may include a circuit board; contact pins electrically connected to the circuit board and being configured and adapted to selectively electrically connect to a complementary electrical plug of the surgical device; a strain gauge supported on and electrically connected to the circuit board, wherein the first rotatable proximal drive shaft extends through the strain gauge; and a slip ring disposed about the distal drive member of the first force/rotation transmitting/converting assembly, wherein the slip ring is in electrical connection with the circuit board, and wherein the slip ring includes electrical contact supported therein for maintaining electrical contact with at least one electrical component within the adapter assembly.

The first proximal drive shaft, the second proximal drive shaft and the third proximal drive shaft of the adapter assembly may be arranged in a common plane with one another.

According to a further aspect of the present disclosure, an adapter assembly is provided and includes a housing configured and adapted for connection with the surgical device and to be in operative communication with each rotatable drive shaft of the surgical device; an outer tube having a proximal end supported by the housing and a distal end configured and adapted for connection with the loading unit, wherein the distal end of the outer tube is in operative communication with each of the axially translatable drive member of the loading unit; force/rotation transmitting/converting assembly for interconnecting a respective one drive shaft of the surgical device and a respective one axially

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translatable drive member of the loading unit; and an electrical assembly supported within the housing and the outer tube thereof.

The electrical assembly includes a circuit board; contact pins electrically connected to the circuit board and being configured and adapted to selectively electrically connect to a complementary electrical plug of the surgical device; a strain gauge supported on and electrically connected to the circuit board, wherein the first rotatable proximal drive shaft extends through the strain gauge; and a slip ring disposed about at least a portion of the first force/rotation transmitting/converting assembly, wherein the slip ring is in electrical connection with the circuit board, and wherein the slip ring includes electrical contact supported therein for maintaining electrical contact with at least one electrical component within the adapter assembly.

The force/rotation transmitting/converting assembly may include a proximal rotation receiving member that is connectable to a respective rotatable drive shaft of the surgical device; and a distal force transmitting member that is connectable to an axially translatable drive member of the loading unit, the distal force transmitting member being connected to the proximal rotation receiving member in such a manner whereby rotation of the proximal rotation receiving member is converted to axial translation of the distal force transmitting member.

In use, the force/rotation transmitting/converting assembly may convert and transmit a rotation of the first rotatable drive shaft of the surgical device to an axial translation of the first axially translatable drive member of the loading unit.

#### BRIEF DESCRIPTION OF THE DRAWINGS

Embodiments of the present disclosure are described herein with reference to the accompanying drawings, wherein:

FIG. 1A is a perspective view of an adapter assembly, in accordance with an embodiment of the present disclosure, interconnected between an exemplary electromechanical surgical device and an end effector assembly;

FIG. 1B is a perspective view illustrating an attachment of a proximal end of the adapter assembly to a distal end of the electromechanical surgical device;

FIG. 2A is a front, perspective view of the adapter assembly of the present disclosure;

FIG. 2B is a rear, perspective view of the adapter assembly of FIG. 2A;

FIG. 3 is a top plan view of the adapter assembly of FIGS. 2A and 2B;

FIG. 4 is a side, elevational view of the adapter assembly of FIGS. 2A and 2B;

FIG. 5 is a rear, perspective view of the adapter assembly of FIGS. 2A and 2B, with some parts thereof separated;

FIG. 6 is a rear, perspective view of the adapter assembly of FIGS. 2A and 2B, with most parts thereof separated;

FIG. 7 is a perspective view of an articulation assembly of the adapter assembly of FIGS. 2A and 2B;

FIG. 8 is an enlarged, perspective view, with parts separated, of the articulation assembly of FIG. 7;

FIG. 9 is a perspective view of the articulation assembly of FIG. 7, shown in a first orientation;

FIG. 10 is a perspective view of the articulation assembly of FIG. 7, shown in a second orientation;

FIG. 11 is a cross-sectional view as taken along section line 11-11 of FIG. 9;

FIG. 12 is a perspective view of an electrical assembly of the adapter assembly of FIGS. 2A and 2B;

FIG. 13 is a perspective view of the electrical assembly of FIG. 12 shown connected to the core housing of the adapter assembly of FIGS. 2A and 2B;

FIG. 14 is a cross-sectional view as taken along section line 14-14 of FIG. 13;

FIG. 15 is a perspective view of a slip ring cannula or sleeve of the adapter assembly of FIGS. 2A and 2B;

FIG. 16 is an enlarged view of the indicated area of detail of FIG. 2B, illustrating an inner housing assembly of the adapter assembly of FIGS. 2A and 2B;

FIG. 17 is a rear, perspective view of the inner housing assembly of FIG. 16 with an outer knob housing half-section and a proximal cap removed therefrom;

FIG. 18 is a rear, perspective view of the inner housing assembly of FIG. 16 with the outer knob housing, the proximal cap and a bushing plate removed therefrom;

FIG. 19 is a rear, perspective view of the inner housing assembly of FIG. 16 with the outer knob housing, the proximal cap, the bushing plate and an inner housing removed therefrom;

FIG. 20 is a rear, perspective view of the an alternative embodiment of inner housing assembly similar to that shown in FIG. 16 with the outer knob housing and the proximal inner housing removed therefrom;

FIG. 21 is a rear, perspective view of the inner housing assembly of FIG. 20 with the outer knob housing, the proximal inner housing and the articulation assembly removed therefrom;

FIG. 22 is a front, perspective view of the inner housing assembly of FIG. 20 with the outer knob housing, the proximal inner housing and the articulation assembly removed therefrom;

FIG. 23 is a front, perspective view of the inner housing assembly of FIG. 20 with the outer knob housing and the proximal inner housing removed therefrom;

FIG. 24 is a cross-sectional view as taken along section line 24-24 of FIG. 2B;

FIG. 25 is an enlarged view of the indicated area of detail of FIG. 24;

FIG. 26 is an enlarged view of the indicated area of detail of FIG. 24, illustrating a lock button being actuated in a proximal direction;

FIG. 27 is a cross-sectional view as taken along section line 27-27 of FIG. 2B;

FIG. 28 is a cross-sectional view as taken along section line 27-27 of FIG. 2B, illustrating actuation of the articulation assembly in a distal direction;

FIG. 29 is a cross-sectional view as taken along section line 29-29 of FIG. 28;

FIG. 30 is a cross-sectional view as taken along section line 30-30 of FIG. 28;

FIG. 31 is a cross-sectional view as taken along section line 31-31 of FIG. 28;

FIG. 32 is a rear, perspective view of a proximal inner housing hub according to the present disclosure;

FIG. 33 is a front, perspective view of the proximal inner housing hub of FIG. 32;

FIG. 34 is a front, perspective view of the proximal inner housing hub of FIGS. 32 and 33 illustrating a first and a second force/rotation transmitting/converting assembly and a reinforcing assembly associated therewith;

FIG. 35 is a front, perspective view of a plate bushing of the proximal inner housing assembly of the present disclosure;

FIG. 36 is a rear, perspective view of the plate bushing of FIG. 35;

FIG. 37 is a rear, perspective view of the proximal inner housing assembly illustrating the plate bushing of FIGS. 35 and 36 attached thereto;

FIG. 38 is a rear, perspective view of the proximal inner housing assembly of FIG. 37 with connector sleeves removed therefrom;

FIG. 39 is a rear, perspective view of the proximal inner housing assembly of FIG. 37 with connector sleeves removed therefrom and the plate bushing shown in phantom;

FIG. 40 is a rear, perspective view of the proximal inner housing assembly of FIG. 37 with connector sleeves removed therefrom;

FIG. 41 is a rear, perspective of the inner housing assembly of FIG. 37 illustrating a support plate, according to another embodiment of the present disclosure, coupled thereto;

FIG. 42 is a rear, perspective of the inner housing assembly of FIG. 41 with the support plate removed therefrom;

FIG. 43 is a front, perspective view of an inner housing assembly according to another embodiment of the present disclosure with the outer knob housing, the proximal inner housing removed therefrom;

FIG. 44 is a rear, perspective view of the inner housing assembly of FIG. 43 with the outer knob housing, the proximal inner housing and the articulation assembly removed therefrom;

FIG. 45 is a perspective view of a bracket assembly of the inner housing assembly of FIGS. 43 and 44;

FIG. 46 is a perspective view of a reinforcing sleeve for use with the inner housing assembly of FIGS. 43 and 44;

FIG. 47 is a perspective view of the inner housing assembly of FIGS. 43 and 44, illustrating the reinforcing sleeve of FIG. 46 supported thereon; and

FIG. 48 is a perspective view, with parts separated, of an exemplary loading unit for use with the surgical device and the adapter of the present disclosure.

#### DETAILED DESCRIPTION OF EMBODIMENTS

Embodiments of the presently disclosed surgical devices, adapter assemblies, and loading unit detection assemblies for surgical devices and/or handle assemblies are described in detail with reference to the drawings, in which like reference numerals designate identical or corresponding elements in each of the several views. As used herein the term “distal” refers to that portion of the adapter assembly or surgical device, or component thereof, farther from the user, while the term “proximal” refers to that portion of the adapter assembly or surgical device, or component thereof, closer to the user.

A surgical device, in accordance with an embodiment of the present disclosure, is generally designated as 100, and is in the form of a powered hand held electromechanical instrument configured for selective attachment thereto of a plurality of different end effectors that are each configured for actuation and manipulation by the powered hand held electromechanical surgical instrument.

As illustrated in FIG. 1A, surgical device 100 is configured for selective connection with an adapter assembly 200, and, in turn, adapter assembly 200 is configured for selective connection with a loading unit 300 (e.g., an end effector, multiple- or single-use loading unit, see FIG. 48). Surgical device 100 and adapter assembly 200, together, may comprise an electromechanical surgical system that is configured and adapted to selectively connect with a loading unit 300 and to actuate loading unit 300.

As illustrated in FIGS. 1A and 1B, surgical device **100** includes a handle housing **102** including a circuit board (not shown) and a drive mechanism (not shown) is situated therein. The circuit board is configured to control the various operations of surgical device **100**. Handle housing **102** defines a cavity therein (not shown) for selective receipt of a rechargeable battery (not shown) therein. The battery is configured to supply power to any of the electrical components of surgical device **100**.

Handle housing **102** includes an upper housing portion **102a** which houses various components of surgical device **100**, and a lower hand grip portion **102b** extending from upper housing portion **102a**. Lower hand grip portion **102b** may be disposed distally of a proximal-most end of upper housing portion **102a**. The location of lower housing portion **102b** relative to upper housing portion **102a** is selected to balance a weight of a surgical device **100** that is connected to or supporting adapter assembly **200** and/or end effector **300**.

Handle housing **102** provides a housing in which the drive mechanism is situated. The drive mechanism is configured to drive shafts and/or gear components in order to perform the various operations of surgical device **100**. In particular, the drive mechanism is configured to drive shafts and/or gear components in order to selectively move a tool assembly **304** of loading unit **300** (see FIGS. 1 and 48) relative to a proximal body portion **302** of loading unit **300**, to rotate loading unit **300** about a longitudinal axis "X" (see FIG. 1A) relative to handle housing **102**, to move/approximate an anvil assembly **306** and a cartridge assembly **308** of loading unit **300** relative to one another, and/or to fire a stapling and cutting cartridge within cartridge assembly **308** of loading unit **300**.

As illustrated in FIG. 1B, handle housing **102** defines a connecting portion **108** configured to accept a corresponding drive coupling assembly **210** of adapter assembly **200**. Specifically, connecting portion **108** of surgical device **100** has a recess **108a** that receives a proximal cap **210a** (FIG. 6) of drive coupling assembly **210** of adapter assembly **200** when adapter assembly **200** is mated to surgical device **100**. Connecting portion **108** houses three rotatable drive connectors **118**, **120**, **122** which are arranged in a common plane or line with one another.

When adapter assembly **200** is mated to surgical device **100**, each of rotatable drive connectors **118**, **120**, **122** of surgical device **100** couples with a corresponding rotatable connector sleeve **218**, **220**, **222** of adapter assembly **200**. (see FIG. 1B). In this regard, the interface between corresponding first drive connector **118** and first connector sleeve **218**, the interface between corresponding second drive connector **120** and second connector sleeve **220**, and the interface between corresponding third drive connector **122** and third connector sleeve **222** are keyed such that rotation of each of drive connectors **118**, **120**, **122** of surgical device **100** causes a corresponding rotation of the corresponding connector sleeve **218**, **220**, **222** of adapter assembly **200**.

The mating of drive connectors **118**, **120**, **122** of surgical device **100** with connector sleeves **218**, **220**, **222** of adapter assembly **200** allows rotational forces to be independently transmitted via each of the three respective connector interfaces. The drive connectors **118**, **120**, **122** of surgical device **100** are configured to be independently rotated by the drive mechanism of surgical device **100**. In this regard, a function selection module (not shown) of the drive mechanism selects which drive connector or connectors **118**, **120**, **122** of surgical device **100** is to be driven by the motor of surgical device **100**.

Since each of drive connectors **118**, **120**, **122** of surgical device **100** has a keyed and/or substantially non-rotatable interface with respective connector sleeves **218**, **220**, **222** of adapter assembly **200**, when adapter assembly **200** is coupled to surgical device **100**, rotational force(s) are selectively transferred from drive connectors of surgical device **100** to adapter assembly **200**.

The selective rotation of drive connector(s) **118**, **120** and/or **122** of surgical device **100** allows surgical device **100** to selectively actuate different functions of loading unit **300**. For example, selective and independent rotation of first drive connector **118** of surgical device **100** corresponds to the selective and independent opening and closing of tool assembly **304** of loading unit **300**, and driving of a stapling/cutting component of tool assembly **304** of loading unit **300**. As an additional example, the selective and independent rotation of second drive connector **120** of surgical device **100** corresponds to the selective and independent articulation of tool assembly **304** of loading unit **300** transverse to longitudinal axis "X" (see FIG. 1A). Additionally, for instance, the selective and independent rotation of third drive connector **122** of surgical device **100** corresponds to the selective and independent rotation of loading unit **300** about longitudinal axis "X" (see FIG. 1A) relative to handle housing **102** of surgical device **100**.

As illustrated in FIG. 1A, handle housing **102** supports a plurality of finger-actuated control buttons, rocker devices and the like for activating various functions of surgical device **100**.

Reference may be made to International Application No. PCT/US2008/077249, filed Sep. 22, 2008 (Inter. Pub. No. WO 2009/039506) and U.S. patent application Ser. No. 12/622,827, filed on Nov. 20, 2009, the entire content of each of which being incorporated herein by reference, for a detailed description of various internal components of and operation of exemplary electromechanical, hand-held, powered surgical instrument **100**.

Turning now to FIGS. 1A-47, adapter assembly **200** includes an outer knob housing **202** and an outer tube **206** extending from a distal end of knob housing **202**. Knob housing **202** and outer tube **206** are configured and dimensioned to house the components of adapter assembly **200**. Outer tube **206** is dimensioned for endoscopic insertion, in particular, that outer tube is passable through a typical trocar port, cannula or the like. Knob housing **202** is dimensioned to not enter the trocar port, cannula of the like. Knob housing **202** is configured and adapted to connect to connecting portion **108** of handle housing **102** of surgical device **100**.

Adapter assembly **200** is configured to convert a rotation of either of drive connectors **118** and **120** of surgical device **100** into axial translation useful for operating a drive assembly **360** and an articulation link **366** of loading unit **300**, as illustrated in FIG. 48 and as will be described in greater detail below. As illustrated in FIGS. 5, 6, 13, 14, 17, 18, 20, 25-34 and 37-40, adapter assembly **200** includes a proximal inner housing assembly **204** rotatably supporting a first rotatable proximal drive shaft **212**, a second rotatable proximal drive shaft **214**, and a third rotatable proximal drive shaft **216** therein. Each proximal drive shaft **212**, **214**, **216** functions as a rotation receiving member to receive rotational forces from respective drive shafts of surgical device **100**, as described in greater detail below.

As described briefly above, inner housing assembly **210** of shaft assembly **200** is also configured to rotatably support first, second and third connector sleeves **218**, **220** and **222**, respectively, arranged in a common plane or line with one another. Each of connector sleeves **218**, **220**, **222** is config-

ured to mate with respective first, second and third drive connectors **118**, **120**, **122** of surgical device **100**, as described above. Each of connector sleeves **218**, **220**, **222** is further configured to mate with a proximal end of respective first, second and third proximal drive shafts **212**, **214**, **216**.

Inner housing assembly **210** also includes, as illustrated in FIGS. **6**, **17**, **27** and **28**, a first, a second and a third biasing member **224**, **226** and **228** disposed distally of respective first, second and third connector sleeves **218**, **220**, **222**. Each of biasing members **224**, **226** and **228** is disposed about respective first, second and third rotatable proximal drive shaft **212**, **214** and **216**. Biasing members **224**, **226** and **228** act on respective connector sleeves **218**, **220** and **222** to help maintain connector sleeves **218**, **220** and **222** engaged with the distal end of respective drive rotatable drive connectors **118**, **120**, **122** of surgical device **100** when adapter assembly **200** is connected to surgical device **100**.

In particular, first, second and third biasing members **224**, **226** and **228** function to bias respective connector sleeves **218**, **220** and **222** in a proximal direction. In this manner, during assembly of adapter assembly **200** to surgical device **100**, if first, second and or third connector sleeves **218**, **220** and/or **222** is/are misaligned with the drive connectors **118**, **120**, **122** of surgical device **100**, first, second and/or third biasing member(s) **224**, **226** and/or **228** are compressed. Thus, when surgical device **100** is operated, drive connectors **118**, **120**, **122** of surgical device **100** will rotate and first, second and/or third biasing member(s) **224**, **226** and/or **228** will cause respective first, second and/or third connector sleeve(s) **218**, **220** and/or **222** to slide back proximally, effectively coupling drive connectors **118**, **120**, **122** of surgical device **100** to first, second and/or third proximal drive shaft(s) **212**, **214** and **216** of inner housing assembly **210**.

Adapter assembly **200** includes a plurality of force/rotation transmitting/converting assemblies, each disposed within inner housing assembly **204** and outer tube **206**. Each force/rotation transmitting/converting assembly is configured and adapted to transmit/convert a speed/force of rotation (e.g., increase or decrease) of first, second and third rotatable drive connectors **118**, **120** and **122** of surgical instrument **100** before transmission of such rotational speed/force to loading unit **300**.

Specifically, as illustrated in FIG. **6**, adapter assembly **200** includes a first, a second and a third force/rotation transmitting/converting assembly **240**, **250**, **260**, respectively, disposed within inner housing **208** and outer tube **206**. Each force/rotation transmitting/converting assembly **240**, **250**, **260** is configured and adapted to transmit or convert a rotation of a first, second and third drive connector **118**, **120**, **122** of surgical device **100** into axial translation of articulation bar **258** of adapter assembly **200**, to effectuate articulation of loading unit **300**; a rotation of a ring gear **266** of adapter assembly **200**, to effectuate rotation of adapter assembly **200**; or axial translation of a distal drive member **248** of adapter assembly **200** to effectuate closing, opening and firing of loading unit **300**.

As shown in FIGS. **5**, **6** and **24-31**, first force/rotation transmitting/converting assembly **240** includes first rotatable proximal drive shaft **212**, which, as described above, is rotatably supported within inner housing assembly **204**. First rotatable proximal drive shaft **212** includes a non-circular or shaped proximal end portion configured for connection with first connector **218** which is connected to respective first connector **118** of surgical device **100**. First rotatable proximal drive shaft **212** includes a distal end portion **212b** having a threaded outer profile or surface.

First force/rotation transmitting/converting assembly **240** further includes a drive coupling nut **244** rotatably coupled to threaded distal end portion **212b** of first rotatable proximal drive shaft **212**, and which is slidably disposed within outer tube **206**. Drive coupling nut **244** is slidably keyed within proximal core tube portion of outer tube **206** so as to be prevented from rotation as first rotatable proximal drive shaft **212** is rotated. In this manner, as first rotatable proximal drive shaft **212** is rotated, drive coupling nut **244** is translated along threaded distal end portion **212b** of first rotatable proximal drive shaft **212** and, in turn, through and/or along outer tube **206**.

First force/rotation transmitting/converting assembly **240** further includes a distal drive member **248** that is mechanically engaged with drive coupling nut **244**, such that axial movement of drive coupling nut **244** results in a corresponding amount of axial movement of distal drive member **248**. The distal end portion of distal drive member **248** supports a connection member **247** configured and dimensioned for selective engagement with a drive member **374** of drive assembly **360** of loading unit **300** (FIG. **47**). Drive coupling nut **244** and/or distal drive member **248** function as a force transmitting member to components of loading unit **300**, as described in greater detail below.

In operation, as first rotatable proximal drive shaft **212** is rotated, due to a rotation of first connector sleeve **218**, as a result of the rotation of the first respective drive connector **118** of surgical device **100**, drive coupling nut **244** is caused to be translated axially along first distal drive shaft **242**. As drive coupling nut **244** is caused to be translated axially along first distal drive shaft **242**, distal drive member **248** is caused to be translated axially relative to outer tube **206**. As distal drive member **248** is translated axially, with connection member **247** connected thereto and engaged with drive member **374** of drive assembly **360** of loading unit **300** (FIG. **47**), distal drive member **248** causes concomitant axial translation of drive member **374** of loading unit **300** to effectuate a closure of tool assembly **304** and a firing of tool assembly **304** of loading unit **300**.

With reference to FIGS. **5-11**, **19** and **23-31**, second drive converter assembly **250** of adapter assembly **200** includes second proximal drive shaft **214** rotatably supported within inner housing assembly **204**. Second rotatable proximal drive shaft **214** includes a non-circular or shaped proximal end portion configured for connection with second connector or coupler **220** which is connected to respective second connector **120** of surgical device **100**. Second rotatable proximal drive shaft **214** further includes a distal end portion **214b** having a threaded outer profile or surface.

Distal end portion **214b** of proximal drive shaft **214** is threadably engaged with an articulation bearing housing **252a** of an articulation bearing assembly **252**. Articulation bearing assembly **252** includes a housing **252a** supporting an articulation bearing **253** having an inner race **253b** that is independently rotatable relative to an outer race **253a**. Articulation bearing housing **252a** has a non-circular outer profile, for example tear-dropped shaped, that is slidably and non-rotatably disposed within a complementary bore **204c** (FIGS. **25**, **26**, **29** and **33**) of inner housing hub **204a**.

Second drive converter assembly **250** of adapter assembly **200** further includes an articulation bar **258** having a proximal portion **258a** secured to inner race **253b** of articulation bearing **253**. A distal portion **258b** of articulation bar **258** includes a slot **258c** therein, which is configured to accept a portion **366**, e.g., a flag, articulation link (FIG. **47**) of loading unit **300**. Articulation bar **258** functions as a force transmit-

ting member to components of loading unit 300, as described in greater detail below.

With further regard to articulation bearing assembly 252, articulation bearing assembly 252 is both rotatable and longitudinally translatable. Additionally, it is envisioned that articulation bearing assembly 252 allows for free, unimpeded rotational movement of loading unit 300 when its jaw members 306, 308 are in an approximated position and/or when jaw members 306, 308 are articulated.

In operation, as second proximal drive shaft 214 is rotated due to a rotation of second connector sleeve 220, as a result of the rotation of the second drive connector 120 of surgical device 100, articulation bearing assembly 252 is caused to be translated axially along threaded distal end portion 214b of second proximal drive shaft 214, which in turn causes articulation bar 258 to be axially translated relative to outer tube 206. As articulation bar 258 is translated axially, articulation bar 258, being coupled to articulation link 366 of loading unit 300, causes concomitant axial translation of articulation link 366 of loading unit 300 to effectuate an articulation of tool assembly 304. Articulation bar 258 is secured to inner race 253b of articulation bearing 253 and is thus free to rotate about the longitudinal axis X-X relative to outer race 253a of articulation bearing 253.

As illustrated in FIGS. 6, 17, 18, 20-23, 25-28, 31 and 37-40 and as mentioned above, adapter assembly 200 includes a third force/rotation transmitting/converting assembly 260 supported in inner housing assembly 204. Third force/rotation transmitting/converting assembly 260 includes a rotation ring gear 266 fixedly supported in and connected to outer knob housing 202. Ring gear 266 defines an internal array of gear teeth 266a (FIG. 6). Ring gear 266 includes a pair of diametrically opposed, radially extending protrusions 266b (FIG. 6) projecting from an outer edge thereof. Protrusions 266b are disposed within recesses defined in outer knob housing 202, such that rotation of ring gear 266 results in rotation of outer knob housing 202, and vice versa.

Third force/rotation transmitting/converting assembly 260 further includes third rotatable proximal drive shaft 216 which, as described above, is rotatably supported within inner housing assembly 204. Third rotatable proximal drive shaft 216 includes a non-circular or shaped proximal end portion configured for connection with third connector 222 which is connected to respective third connector 122 of surgical device 100. Third rotatable proximal drive shaft 216 includes a spur gear 216a keyed to a distal end thereof. A reversing spur gear 264 inter-engages spur gear 216a of third rotatable proximal drive shaft 216 to gear teeth 266a of ring gear 266.

In operation, as third rotatable proximal drive shaft 216 is rotated, due to a rotation of third connector sleeve 222, as a result of the rotation of the third drive connector 122 of surgical device 100, spur gear 216a of third rotatable proximal drive shaft 216 engages reversing gear 264 causing reversing gear 264 to rotate. As reversing gear 264 rotates, ring gear 266 also rotates thereby causing outer knob housing 202 to rotate. As outer knob housing 202 is rotated, outer tube 206 is caused to be rotated about longitudinal axis "X" of adapter assembly 200. As outer tube 206 is rotated, loading unit 300, that is connected to a distal end portion of adapter assembly 200, is also caused to be rotated about a longitudinal axis of adapter assembly 200.

Adapter assembly 200 further includes, as seen in FIGS. 1B, 3-5, 16, 17, 20 and 24-26, an attachment/detachment button 272 supported thereon. Specifically, button 272 is supported on drive coupling assembly 210 of adapter assem-

bly 200 and is biased by a biasing member 274 to an un-actuated condition. Button 272 includes lip or ledge 272a formed therewith that is configured to snap behind a corresponding lip or ledge 108b defined along recess 108a of connecting portion 108 of surgical device 100. In use, when adapter assembly 200 is connected to surgical device 100, lip 272a of button 272 is disposed behind lip 108b of connecting portion 108 of surgical device 100 to secure and retain adapter assembly 200 and surgical device 100 with one another. In order to permit disconnection of adapter assembly 200 and surgical device 100 from one another, button 272 is depressed or actuated, against the bias of biasing member 274, to disengage lip 272a of button 272 and lip 108b of connecting portion 108 of surgical device 100.

With reference to FIGS. 1A, 2A, 2B, 3-5 and 24-26, adapter assembly 200 further includes a lock mechanism 280 for fixing the axial position and radial orientation of distal drive member 248. Lock mechanism 280 includes a button 282 slidably supported on outer knob housing 202. Lock button 282 is connected to an actuation bar 284 that extends longitudinally through outer tube 206. Actuation bar 284 moves upon a movement of lock button 282. Upon a predetermined amount of movement of lock button 282, a distal end of actuation bar 284 may move into contact with a lock out (not shown), which causes the lock out to cam a camming member 288 (FIG. 24) from a recess 249 in distal drive member 248. When camming member 288 is in engagement with recess 249 (e.g., at least partially within recess 249, see FIGS. 6 and 24), the engagement between camming member 288 and distal drive member 248 effectively locks the axial and rotational position of end effector 300 that is engaged with connection member 247.

In operation, in order to lock the position and/or orientation of distal drive member 248, a user moves lock button 282 from a distal position to a proximal position (FIGS. 25 and 26), thereby causing the lock out (not shown) to move proximally such that a distal face of the lock out moves out of contact with camming member 288, which causes camming member 288 to cam into recess 249 of distal drive member 248. In this manner, distal drive member 248 is prevented from distal and/or proximal movement. When lock button 282 is moved from the proximal position to the distal position, the distal end of actuation bar 284 moves distally into the lock out, against the bias of a biasing member (not shown), to force camming member 288 out of recess 249, thereby allowing unimpeded axial translation and radial movement of distal drive member 248.

Reference may be made to U.S. patent application Ser. No. 13/875,571, filed on May 2, 2013, the entire content of which is incorporated herein by reference, for a more detailed discussion of the construction and operation of lock mechanism 280.

With reference to FIGS. 1B, 6, 12-15 and 25-28, adapter assembly 200 includes an electrical assembly 290 supported on and in outer knob housing 202 and inner housing assembly 204. Electrical assembly 290 includes a plurality of electrical contact pins 292, supported on a circuit board 294, for electrical connection to a corresponding electrical plug 190 disposed in connecting portion 108 of surgical device 100. Electrical contacts 290 serve to allow for calibration and communication of life-cycle information to the circuit board of surgical device 100 via electrical plugs 190 that are electrically connected to the circuit board (not shown) of surgical device 100.

Electrical assembly 290 further includes a strain gauge 296 electrically connected to circuit board 294. Strain gauge

296 is provided with a notch 296a which is configured and adapted to receive stem 204d of hub 204a of inner housing assembly 204. Stem 204d of hub 204a functions to restrict rotational movement of strain gauge 296. As illustrated in FIGS. 25-28, first rotatable proximal drive shaft 212 extends through strain gauge 296. Strain gauge 296 provides a closed-loop feedback to a firing/clamping load exhibited by first rotatable proximal drive shaft 212.

Electrical assembly 290 also includes a slip ring 298 disposed core tube of tube 206. Slip ring 298 is in electrical connection with circuit board 294. Slip ring 298 functions to permit rotation of first rotatable proximal drive shaft 212 and axial translation of drive coupling nut 244 while still maintaining electrical contact of electrical contact rings 298a thereof with at least another electrical component within adapter assembly 200, and while permitting the other electrical components to rotate about first rotatable proximal drive shaft 212 and drive coupling nut 244.

Electrical assembly 290 may include a slip ring cannula or sleeve 299 positioned core tube of tube 206 to protect and/or shield any wires extending from slip ring 298.

Turning now to FIGS. 6, 11, 14, 32 and 33, inner housing assembly 204 has been designed to reduce incidents of racking of second proximal drive shaft 214 as drive shaft 214 rotates to axially translate articulation bearing assembly 252. Inner housing assembly 204 includes a hub 204a having a distally oriented annular wall 204b defining a substantially circular outer profile, and defining a substantially tear-drop shaped inner recess or bore 204c. Bore 204c of hub 204a is shaped and dimensioned to slidably receive articulation bearing assembly 252 therewithin.

Inner housing assembly 204 includes a ring plate 254a (FIG. 34) secured to a distal face of distally oriented annular wall 204b of hub 204a. Plate 254a defines an aperture 254e therethrough that is sized and formed therein so as to be aligned with second proximal drive shaft 214 and to rotatably receive a distal tip 214c of second proximal drive shaft 214. In this manner, distal tip 214c of second proximal drive shaft 214 is supported and prevented from moving radially away from a longitudinal rotational axis of second proximal drive shaft 214 as second proximal drive shaft 214 is rotated to axially translate articulation bearing assembly 252.

As illustrated in FIGS. 14, 32, 39 and 40, hub 204a defines a feature (e.g., a stem or the like) 204d projecting therefrom which functions to engage notch 296a of strain gauge 296 of electrical assembly 290 to measure forces experienced by shaft 212 as surgical device 100 is operated.

With reference to FIGS. 35-40, a plate bushing 230 of inner housing assembly 204 is shown and described. Plate bushing 230 extends across hub 204a of inner housing assembly 204 and is secured to hub 204a by fastening members. Plate bushing 230 defines three apertures 230a, 230b, 230c that are aligned with and rotatably receive respective first, second and third proximal drive shafts 212, 214, 216 therein. Plate bushing 230 provides a surface against which first, second and third biasing members 224, 226 and 228 come into contact or rest against.

While plate bushing 230 has been shown and described as being a unitary monolithic piece, as illustrated in FIGS. 6 and 37-40, it is envisioned and within the scope of the present application that plate bushing 230 may be separated into several parts including, and not limited to, as seen in FIGS. 40-42, a support plate 230' extending across drive shafts 212, 214, 216, and a separate bushing for each of drive shafts 212, 214, 216 and disposed between the support plate 230' and hub 204a of inner housing assembly 204. Support plate 230' may include a pair of slots 230a', 230b' formed

therein, which are configured and adapted to receive tabs 296b of strain gauge 296 that project axially therefrom.

Turning now to FIGS. 43-47, an inner housing assembly 204' according to another embodiment of the present disclosure is shown and will be described. In order to reduce incidents of racking (i.e., distal end 214b of second proximal drive shaft 214 moving radially away from a longitudinal rotational axis thereof) of second proximal drive shaft 214 as drive shaft 214 rotates to axially translate articulation bearing assembly 252, inner housing assembly 204' may include a reinforcement frame or bracket assembly 254'. Bracket assembly 254' includes a first plate 254a' and a second plate 254b' integrally connected to and spaced a distance from first plate 254a' by a plurality of connecting rods 254c' extending therebetween.

First plate 254a' is disposed adjacent to or in close proximity to ring gear 266 and defines an aperture 254d' therethrough. Aperture 254d' is sized and formed in first plate 254a' so as to be aligned with second proximal drive shaft 214 and to permit second proximal drive shaft 214 to freely rotate therewithin. Second plate 254b' is spaced from first plate 254a' so as to be disposed at a distal free end of second proximal drive shaft 214. Second plate 254b' defines an aperture 254e' therethrough. Aperture 254e' is sized and formed in second plate or flange 254b' so as to be aligned with second proximal drive shaft 214 and to rotatably receive a distal tip 214c of second proximal drive shaft 214.

In this manner, distal tip 214c of second proximal drive shaft 214 is supported and prevented from moving radially away from a longitudinal rotational axis of second proximal drive shaft 214 as second proximal drive shaft 214 is rotated to axially translate articulation bearing assembly 252.

As illustrated in FIGS. 38, 46 and 47, inner housing assembly 204' may include a reinforcing sleeve 255' disposed about bracket assembly 254' to further reinforce bracket assembly 254'. It is contemplated in an embodiment that reinforcing sleeve 255' may be interposed between first plate 254a' and second plate 254b' of bracket assembly 254'. It is further contemplated that reinforcing sleeve 255' may be interposed between second plate 254b' and a distally oriented face of proximal inner housing assembly 204'.

In accordance with the present disclosure, an overall length of adapter assembly 200 has been reduced as compared to prior adapter assemblies that have been developed to transmit/convert forces/rotations from surgical device 100 to loading unit 300. By reducing an overall length of adapter assembly 200, a center of gravity of an assembled surgical device 100, adapter assembly 200 and loading unit 300 has been shifted proximally as compared to a center of gravity of an assembled surgical device 100, a prior adapter assembly and a loading unit 300. As such, a level of comfort to the end user in using the electromechanical surgical system of the present disclosure has been increased, and a level of fatigue has been decreased.

In operation, when a button of surgical device 100 is activated by the user, the software checks predefined conditions. If conditions are met, the software controls the motors and delivers mechanical drive to the attached surgical stapler, which can then open, close, rotate, articulate or fire depending on the function of the pressed button. The software also provides feedback to the user by turning colored lights on or off in a defined manner to indicate the status of surgical device 100, adapter assembly 200 and/or loading unit 300.

Reference may be made to U.S. Patent Publication No. 2009/0314821, filed on Aug. 31, 2009, entitled "TOOL ASSEMBLY FOR A SURGICAL STAPLING DEVICE" for



a detailed discussion of the construction and operation of loading unit **300**, as illustrated in FIGS. **1** and **48**.

Any of the components described herein may be fabricated from either metals, plastics, resins, composites or the like taking into consideration strength, durability, wearability, weight, resistance to corrosion, ease of manufacturing, cost of manufacturing, and the like.

It will be understood that various modifications may be made to the embodiments of the presently disclosed adapter assemblies. Therefore, the above description should not be construed as limiting, but merely as exemplifications of embodiments. Those skilled in the art will envision other modifications within the scope and spirit of the present disclosure.

What is claimed is:

**1.** An adapter assembly for selectively interconnecting a surgical loading unit that is configured to perform a function and a surgical device that is configured to actuate the loading unit, the loading unit including at least one axially translatable drive member, and the surgical device including at least one rotatable drive shaft, the adapter assembly comprising: a housing configured and adapted for connection with the surgical device and to be in operative communication with each of the at least one rotatable drive shaft of the surgical device; an outer tube having a proximal end supported by the housing and a distal end configured and adapted for connection with the loading unit, wherein the distal end of the outer tube is in operative communication with each of the at least one axially translatable drive member of the loading unit; and a plurality of force/rotation

transmitting/converting assemblies, each of the plurality of force/rotation

transmitting/converting assemblies configured for interconnecting a respective one of the at least one rotatable drive shaft of the surgical device and a respective one of the at least one axially translatable drive member of the loading unit, wherein each of the plurality of force/rotation transmitting/converting assemblies includes: a proximal rotation receiving member that is connectable to the respective one of the at least one rotatable drive shaft of the surgical device, each of the proximal rotation receiving members being arranged in a longitudinally extending common plane with one another; and a distal force transmitting member that is connectable to the respective one of the at least one axially translatable drive member of the loading unit, each of the distal force transmitting members being connected to each of the proximal rotation receiving members, respectively, in such a manner whereby rotation of the proximal rotation receiving member is converted to axial translation of the distal force transmitting member; wherein the plurality of force/rotation transmitting/converting assemblies converts and transmits a rotation of the respective one of the at least one rotatable drive shaft of the surgical device to an axial translation of the respective one of the at least one axially translatable drive member of the loading unit; wherein the plurality of force/rotation

transmitting/converting assemblies includes a first force/rotation transmitting/converting assembly; wherein the proximal rotation receiving member of the first force/rotation transmitting/converting assembly includes a first proximal drive shaft defining a threaded distal end; and wherein the distal force transmitting member of the first force/rotation transmitting/converting assembly includes a distal drive member threadably connected to the threaded distal end of the first proximal drive shaft,

wherein the first proximal drive shaft and the distal drive member are axially aligned with one another and with a rotational axis of the respective rotatable drive shaft of the surgical device.

**2.** The adapter assembly according to claim **1**, wherein rotation of the rotatable drive shaft of the surgical device, associated with the first force/rotation transmitting/converting assembly, results in rotation of the first rotatable drive shaft of the first force/rotation transmitting/converting assembly which results in axial translation of the distal drive member of the first force/rotation transmitting/converting assembly.

**3.** The adapter assembly according to claim **1**, wherein the plurality of force/rotation transmitting/converting assemblies includes a second force/rotation transmitting/converting assembly; wherein the proximal rotation receiving member of the second force/rotation transmitting/converting assembly includes a second proximal drive shaft defining a threaded distal end; and wherein the distal force transmitting member of the second force/rotation transmitting/converting assembly includes a bearing assembly having an outer race threadably connected to the threaded distal end of the second proximal drive shaft and being non-rotatably disposed within the housing.

**4.** The adapter assembly according to claim **3**, wherein the bearing assembly includes an inner race, and wherein the distal force transmitting member of the second force/rotation transmitting/converting assembly includes an articulation bar having a proximal end secured to the inner race of the bearing assembly, and a distal end configured to selectively engage a second axially translatable drive member of the loading unit.

**5.** The adapter assembly according to claim **3**, wherein at least a portion of the first force/rotation transmitting/converting assembly extends through the bearing assembly of the second force/rotation transmitting/converting assembly.

**6.** The adapter assembly according to claim **5**, wherein the articulation bar is rotatable about the first force/rotation transmitting/converting assembly.

**7.** The adapter assembly according to claim **3**, wherein rotation of the respective one of the at least one rotatable drive shaft of the surgical device, associated with the second force/rotation transmitting/converting assembly, results in rotation of the second rotatable drive shaft of the second force/rotation transmitting/converting assembly which results in axial translation of the articulation bar of the second force/rotation transmitting/converting assembly.

**8.** The adapter assembly according to claim **7**, wherein the plurality of force/rotation transmitting/converting assemblies includes a third force/rotation transmitting/converting assembly; wherein the proximal rotation receiving member of the third force/rotation transmitting/converting assembly includes a third proximal drive shaft having a spur gear supported on a distal end thereof; and wherein the distal force transmitting member of the third force/rotation transmitting/converting assembly includes a ring gear fixedly supported in the housing and being in gearing connection with the spur gear.

**9.** The adapter assembly according to claim **8**, wherein rotation of the respective one of the at least one rotatable drive shaft of the surgical device, associated with the third force/rotation transmitting/converting assembly, results in rotation of the third rotatable drive shaft of the third force/rotation transmitting/converting assembly which results in rotation of the ring gear of the third force/rotation transmitting/converting assembly.

**10.** The adapter assembly according to claim **8**, further comprising an electrical assembly supported within at least one of the housing and the outer tube, the electrical assembly including:

- a circuit board; 5
- at least one contact pin electrically connected to the circuit board and being configured and adapted to selectively electrically connect to a complementary electrical plug of the surgical device;
- a strain gauge supported on and electrically connected to the circuit board, wherein the first rotatable proximal drive shaft extends through the strain gauge; and 10
- a slip ring disposed about the distal drive member of the first force/rotation transmitting/converting assembly, wherein the slip ring is in electrical connection with the circuit board, and wherein the slip ring includes electrical contact supported therein for maintaining electrical contact with at least one electrical component within the adapter assembly. 15

**11.** The adapter assembly according to claim **8**, wherein the second proximal drive shaft is spaced a first radial distance from the first proximal drive shaft, and the third proximal drive shaft is spaced a second radial distance from the first proximal drive shaft, wherein the second radial distance is equal to the first radial distance. 20  
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**12.** The adapter assembly according to claim **1**, wherein each of the proximal rotation receiving members is arranged to be radially separated from one another.

**13.** The adapter assembly according to claim **1**, wherein the common plane is defined by a rotational axis of each of the proximal rotation receiving members. 30

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