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(54) **MICROFLUIDIC DEVICES AND METHODS OF USE IN THE FORMATION AND CONTROL OF NANOREACTORS**

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(56) **References Cited**

U.S. PATENT DOCUMENTS

2,097,692 A 11/1937 Fiegel
2,164,172 A 6/1939 Dalton
(Continued)

FOREIGN PATENT DOCUMENTS

AU 2177292 A 1/1993
AU 677197 B2 4/1997
(Continued)

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OTHER PUBLICATIONS

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(Continued)

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(57) **ABSTRACT**

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The present invention provides novel microfluidic devices and methods that are useful for performing high-throughput screening assays and combinatorial chemistry. The invention provides for aqueous based emulsions containing uniquely labeled cells, enzymes, nucleic acids, etc., wherein the emulsions further comprise primers, labels, probes, and other reactants. An oil based carrier-fluid envelopes the emulsion library on a microfluidic device, such that a continuous channel provides for flow of the immiscible fluids, to accomplish pooling, coalescing, mixing, sorting, detection, etc., of the emulsion library.

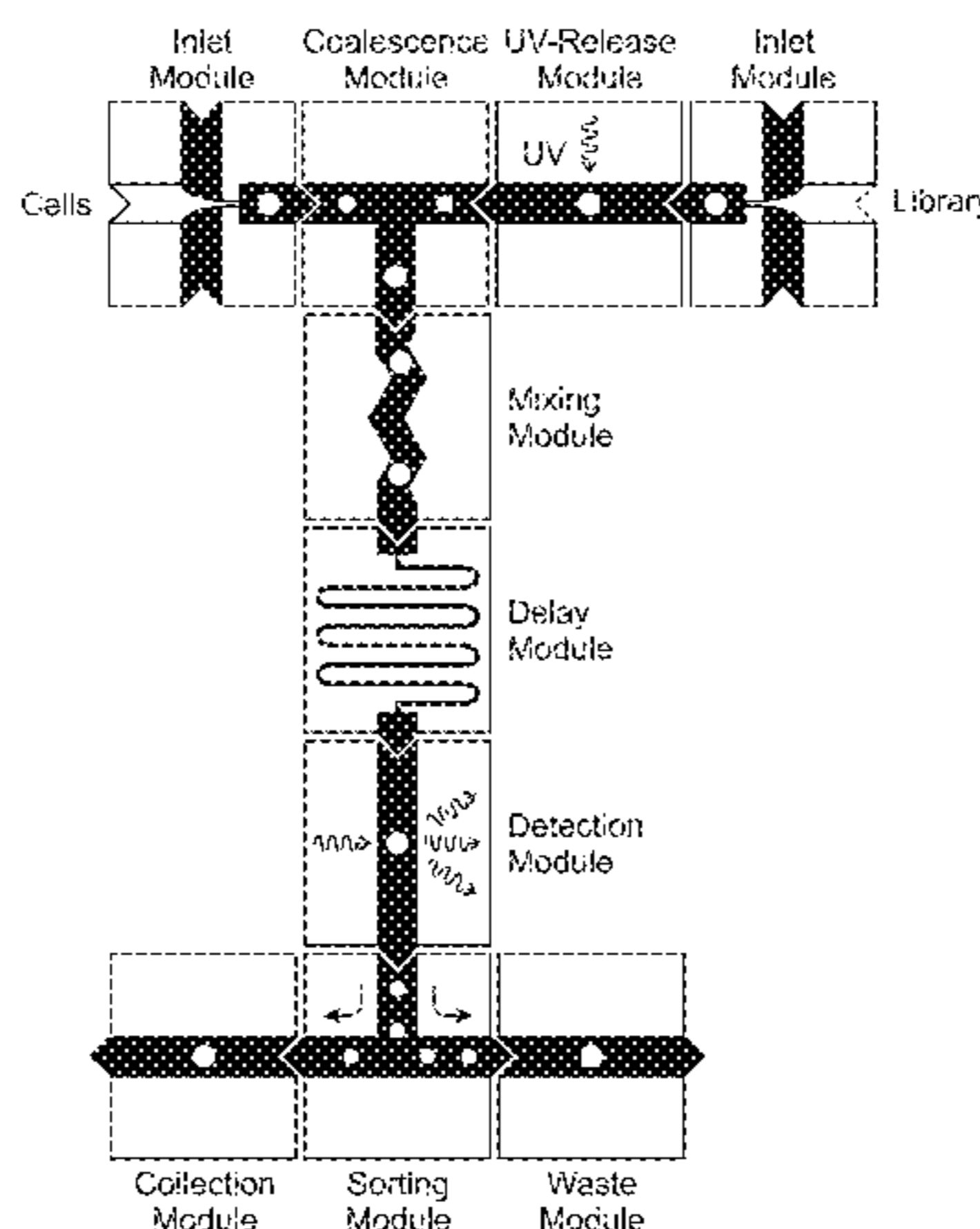
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(56)

References Cited

U.S. PATENT DOCUMENTS

2,636,855 A 4/1953 Schwarz
2,656,508 A 10/1953 Coulter
2,692,800 A 10/1954 Nichols et al.
2,797,149 A 6/1957 Skeggs
2,879,141 A 3/1959 Skeggs
2,971,700 A 2/1961 Peeps
3,479,141 A 11/1969 Smythe et al.
3,608,821 A 9/1971 Simm et al.
3,698,635 A 10/1972 Sickles
3,784,471 A 1/1974 Kaiser
3,816,331 A 6/1974 Brown, Jr. et al.
3,930,061 A 12/1975 Scharfenberger
3,960,187 A 6/1976 Stock et al.
3,980,541 A 9/1976 Aine
3,982,541 A 9/1976 L'Esperance, Jr.
4,014,469 A 3/1977 Sato
4,022,575 A 5/1977 Hansen et al.
4,034,966 A 7/1977 Suh et al.
4,059,552 A 11/1977 Zweigle et al.
4,091,042 A 5/1978 Alexanderson et al.
4,117,550 A 9/1978 Folland et al.
4,130,394 A 12/1978 Negersmith
4,210,809 A 7/1980 Pelavin
4,253,846 A 3/1981 Smythe et al.
4,266,721 A 5/1981 Sickles
4,279,345 A 7/1981 Allred
4,297,345 A 10/1981 Howarth
4,315,754 A 2/1982 Ruzicka et al.
4,378,957 A 4/1983 Malkin et al.
4,383,767 A 5/1983 Jido
4,439,980 A 4/1984 Biblarz et al.
4,508,265 A 4/1985 Jido
4,533,634 A 8/1985 Maldonado et al.
4,585,209 A 4/1986 Aine et al.
4,618,476 A 10/1986 Columbus
4,675,285 A 6/1987 Clark et al.
4,676,274 A 6/1987 Brown
4,683,195 A 7/1987 Mullis et al.
4,683,202 A 7/1987 Mullis
4,739,044 A 4/1988 Stabinsky
4,757,141 A 7/1988 Fung et al.
4,767,515 A 8/1988 Scott et al.
4,767,929 A 8/1988 Valentine
4,779,805 A 10/1988 Jackson et al.
4,795,330 A 1/1989 Noakes et al.
4,801,086 A 1/1989 Noakes
4,801,529 A 1/1989 Perlman
4,829,996 A 5/1989 Noakes et al.
4,853,336 A 8/1989 Saros et al.
4,856,363 A 8/1989 LaRocca et al.
4,859,363 A 8/1989 Davis et al.
4,865,444 A 9/1989 Green et al.
4,883,750 A 11/1989 Whiteley et al.
4,908,112 A 3/1990 Pace
4,931,225 A 6/1990 Cheng
4,941,959 A 7/1990 Scott
4,962,885 A 10/1990 Coffee
4,963,498 A 10/1990 Hillman et al.
4,981,580 A 1/1991 Auer
4,996,004 A 2/1991 Bucheler et al.
5,091,652 A 2/1992 Mathies et al.

(56)

References Cited

U.S. PATENT DOCUMENTS

5,096,615 A	3/1992	Prescott et al.	5,840,506 A	11/1998	Giordano
5,122,360 A	6/1992	Harris et al.	5,846,719 A	12/1998	Brenner et al.
5,149,625 A	9/1992	Church et al.	5,849,491 A	12/1998	Radomski et al.
5,180,662 A	1/1993	Sitkovsky	5,851,769 A	12/1998	Gray et al.
5,185,099 A	2/1993	Delpuech et al.	5,858,187 A	1/1999	Ramsey et al.
5,188,290 A	2/1993	Gebauer et al.	5,858,655 A	1/1999	Arnold
5,188,291 A	2/1993	Cross	5,858,670 A	1/1999	Lam et al.
5,192,659 A	3/1993	Simons	5,863,722 A	1/1999	Brenner
5,204,112 A	4/1993	Hope et al.	5,868,322 A	2/1999	Loucks, Jr. et al.
5,207,973 A	5/1993	Harris et al.	5,872,010 A	2/1999	Karger et al.
5,241,159 A	8/1993	Chatterjee et al.	5,876,771 A	3/1999	Sizer et al.
5,260,466 A	11/1993	McGibbon	5,880,071 A	3/1999	Parce et al.
5,262,027 A	11/1993	Scott	5,882,680 A	3/1999	Suzuki et al.
5,270,163 A	12/1993	Gold et al.	5,882,856 A	3/1999	Shuber
5,296,375 A	3/1994	Kricka et al.	5,884,846 A	3/1999	Tan
5,304,487 A	4/1994	Wilding et al.	5,887,755 A	3/1999	Hood, III
5,310,653 A	5/1994	Hanausek-Walaszek et al.	5,888,746 A	3/1999	Tabiti et al.
5,313,009 A	5/1994	Guenkel et al.	5,888,778 A	3/1999	Shuber
5,333,675 A	8/1994	Mullis et al.	5,904,933 A	5/1999	Riess et al.
5,344,594 A	9/1994	Sheridon	5,921,678 A	7/1999	Desai et al.
5,376,252 A	12/1994	Ekstrom et al.	5,927,852 A	7/1999	Serafin
5,378,957 A	1/1995	Kelly	5,928,870 A	7/1999	Lapidus et al.
5,397,605 A	3/1995	Barbieri	5,932,100 A	8/1999	Yager et al.
5,399,461 A	3/1995	Van et al.	5,935,331 A	8/1999	Naka et al.
5,399,491 A	3/1995	Kacian et al.	5,942,056 A	8/1999	Singh
5,403,617 A	4/1995	Haaland	5,942,443 A	8/1999	Parce et al.
5,413,924 A	5/1995	Kosak et al.	5,958,203 A	9/1999	Parce et al.
5,417,235 A	5/1995	Wise et al.	5,972,187 A	10/1999	Parce et al.
5,427,946 A	6/1995	Kricka et al.	5,980,936 A	11/1999	Krafft et al.
5,445,934 A	8/1995	Fodor et al.	5,989,815 A	11/1999	Skolnick et al.
5,452,878 A	9/1995	Gravesen et al.	5,989,892 A	11/1999	Nishimaki et al.
5,452,955 A	9/1995	Lundstrom	5,995,341 A	11/1999	Tanaka et al.
5,454,472 A	10/1995	Benecke et al.	5,997,636 A	12/1999	Gamarnik et al.
5,460,945 A	10/1995	Springer et al.	6,008,003 A	12/1999	Haak-Frendscho et al.
5,468,613 A	11/1995	Erlich et al.	6,023,540 A	2/2000	Walt et al.
5,475,096 A	12/1995	Gold et al.	6,028,066 A	2/2000	Unger
5,475,610 A	12/1995	Atwood et al.	6,042,709 A	3/2000	Parce et al.
5,480,614 A	1/1996	Kamahori	6,045,755 A	4/2000	Lebl et al.
5,486,335 A	1/1996	Wilding et al.	6,046,056 A	4/2000	Parce et al.
5,498,392 A	3/1996	Wilding et al.	6,048,551 A	4/2000	Hilfinger et al.
5,500,415 A	3/1996	Dollat et al.	6,068,199 A	5/2000	Coffee
5,503,851 A	4/1996	Mank et al.	6,074,879 A	6/2000	Zelmanovic et al.
5,512,131 A	4/1996	Kumar et al.	6,080,295 A	6/2000	Parce et al.
5,516,635 A	5/1996	Ekins et al.	6,086,740 A	7/2000	Kennedy
5,518,709 A	5/1996	Sutton et al.	6,096,495 A	8/2000	Kasai et al.
5,523,162 A	6/1996	Franz et al.	6,103,537 A	8/2000	Ullman et al.
5,587,128 A	12/1996	Wilding et al.	6,105,571 A	8/2000	Coffee
5,589,136 A	12/1996	Northrup et al.	6,105,877 A	8/2000	Coffee
5,602,756 A	2/1997	Atwood et al.	6,107,059 A	8/2000	Hart
5,604,097 A	2/1997	Brenner	6,116,516 A	9/2000	Ganan-Calvo
5,610,016 A	3/1997	Sato et al.	6,118,849 A	9/2000	Tanimori et al.
5,612,188 A	3/1997	Shuler et al.	6,119,953 A	9/2000	Ganan-Calvo et al.
5,616,478 A	4/1997	Chetverin et al.	6,120,666 A	9/2000	Jacobson et al.
5,617,997 A	4/1997	Kobayashi et al.	6,124,388 A	9/2000	Takai et al.
5,635,358 A	6/1997	Wilding et al.	6,124,439 A	9/2000	Friedman et al.
5,636,400 A	6/1997	Young	6,130,052 A	10/2000	Van Baren et al.
5,641,658 A	6/1997	Adams et al.	6,130,098 A	10/2000	Handique et al.
5,643,729 A	7/1997	Taniguchi et al.	6,137,214 A	10/2000	Raina
5,655,517 A	8/1997	Coffee	6,138,077 A	10/2000	Brenner
5,656,155 A	8/1997	Norcross et al.	6,139,303 A	10/2000	Reed et al.
5,656,493 A	8/1997	Mullis et al.	6,140,053 A	10/2000	Koster
5,661,222 A	8/1997	Hare	6,143,496 A	11/2000	Brown et al.
5,662,874 A	9/1997	David	6,146,828 A	11/2000	Lapidus et al.
5,670,325 A	9/1997	Lapidus et al.	6,149,789 A	11/2000	Benecke et al.
5,681,600 A	10/1997	Antinone et al.	6,150,180 A	11/2000	Parce et al.
5,695,934 A	12/1997	Brenner	6,150,516 A	11/2000	Brenner et al.
5,726,026 A	3/1998	Wilding et al.	6,165,778 A	12/2000	Kedar
5,726,404 A	3/1998	Brody	6,171,796 B1	1/2001	An et al.
5,733,526 A	3/1998	Trevino et al.	6,171,850 B1	1/2001	Nagle et al.
5,739,036 A	4/1998	Parris	6,172,214 B1	1/2001	Brenner
5,744,366 A	4/1998	Kricka et al.	6,172,218 B1	1/2001	Brenner
5,750,988 A	5/1998	Apffel et al.	6,174,160 B1	1/2001	Lee et al.
5,762,775 A	6/1998	DePaoli et al.	6,174,469 B1	1/2001	Ganan-Calvo
5,779,868 A	7/1998	Parce et al.	6,177,479 B1	1/2001	Nakajima et al.
5,783,431 A	7/1998	Peterson et al.	6,180,372 B1	1/2001	Franzen
			6,184,012 B1	2/2001	Neri et al.
			6,187,214 B1	2/2001	Ganan-Calvo
			6,189,803 B1	2/2001	Ganan-Calvo
			6,196,525 B1	3/2001	Ganan-Calvo

(56)

References Cited

U.S. PATENT DOCUMENTS

6,197,335 B1	3/2001	Sherman	6,520,425 B1	2/2003	Reneker
6,197,835 B1	3/2001	Ganan-Calvo	6,524,456 B1	2/2003	Ramsey et al.
6,203,993 B1	3/2001	Shuber et al.	6,540,395 B2	4/2003	Muhlbauer et al.
6,207,372 B1	3/2001	Shuber	6,540,895 B1	4/2003	Spence et al.
6,207,397 B1 *	3/2001	Lynch G01N 33/542 435/7.1	6,551,836 B1	4/2003	Chow et al.
6,210,396 B1	4/2001	MacDonald et al.	6,553,944 B1	4/2003	Allen et al.
6,210,891 B1	4/2001	Nyren et al.	6,553,960 B1	4/2003	Yoshikawa et al.
6,210,896 B1	4/2001	Chan	6,554,202 B2	4/2003	Ganan-Calvo
6,214,558 B1	4/2001	Shuber et al.	6,557,334 B2	5/2003	Jager
6,221,654 B1	4/2001	Quake et al.	6,557,834 B2	5/2003	Ganan-Calvo
6,227,466 B1	5/2001	Hartman et al.	6,558,944 B1	5/2003	Parce et al.
6,234,402 B1	5/2001	Ganan-Calvo	6,558,960 B1	5/2003	Parce et al.
6,235,383 B1	5/2001	Hong et al.	6,560,030 B2	5/2003	Legrand et al.
6,235,475 B1	5/2001	Brenner et al.	6,565,010 B2	5/2003	Anderson et al.
6,241,159 B1	6/2001	Ganan-Calvo et al.	6,569,631 B1	5/2003	Pantoliano et al.
6,243,373 B1	6/2001	Turock	6,576,420 B1	6/2003	Carson et al.
6,248,378 B1	6/2001	Ganan-Calvo	6,591,852 B1	7/2003	McNeely et al.
6,251,661 B1	6/2001	Urabe et al.	6,592,321 B2	7/2003	Bonker et al.
6,252,129 B1	6/2001	Coffee	6,592,821 B1	7/2003	Wada et al.
6,258,568 B1	7/2001	Nyren	6,601,613 B2	8/2003	McNeely et al.
6,258,858 B1	7/2001	Nakajima et al.	6,608,726 B2	8/2003	Legrand et al.
6,263,222 B1	7/2001	Diab et al.	6,610,499 B1	8/2003	Fulwyler et al.
6,266,459 B1	7/2001	Walt et al.	6,614,598 B1	9/2003	Quake et al.
6,267,353 B1	7/2001	Friedline et al.	6,627,603 B1	9/2003	Bibette et al.
6,267,858 B1	7/2001	Parce et al.	6,630,006 B2	10/2003	Santarsiero et al.
6,268,165 B1	7/2001	O'Brien	6,630,353 B1	10/2003	Parce et al.
6,268,222 B1	7/2001	Chandler et al.	6,632,619 B1	10/2003	Harrison et al.
6,274,320 B1	8/2001	Rothberg et al.	6,637,463 B1	10/2003	Lei et al.
6,274,337 B1	8/2001	Parce et al.	6,638,749 B1	10/2003	Beckman et al.
6,280,948 B1	8/2001	Guilfoyle et al.	6,645,432 B1	11/2003	Anderson et al.
6,294,344 B1	9/2001	O'Brien	6,646,253 B1	11/2003	Rohwer et al.
6,296,020 B1	10/2001	McNeely et al.	6,653,626 B2	11/2003	Fischer et al.
6,296,673 B1	10/2001	Santarsiero et al.	6,656,267 B2	12/2003	Newman
6,299,145 B1	10/2001	Ganan-Calvo	6,659,370 B1	12/2003	Inoue
6,301,055 B1	10/2001	Legrand et al.	6,660,252 B2	12/2003	Matathia et al.
6,306,659 B1	10/2001	Parce et al.	6,670,142 B2	12/2003	Lau et al.
6,310,354 B1	10/2001	Hanninen et al.	6,679,441 B1	1/2004	Borra et al.
6,310,653 B1	10/2001	Malcolm, Jr. et al.	6,680,178 B2	1/2004	Harris et al.
6,316,208 B1	11/2001	Roberts et al.	6,682,890 B2	1/2004	Mack et al.
6,316,213 B1	11/2001	O'Brien	6,717,136 B2	4/2004	Andersson et al.
6,318,640 B1	11/2001	Coffee	6,729,561 B2	5/2004	Hirae et al.
6,336,463 B1	1/2002	Ohta	6,739,036 B2	5/2004	Koike et al.
6,344,325 B1	2/2002	Quake et al.	6,744,046 B2	6/2004	Valaskovic et al.
6,352,828 B1	3/2002	Brenner	6,752,922 B2	6/2004	Huang et al.
6,355,193 B1	3/2002	Stott	6,753,147 B2	6/2004	Vogelstein et al.
6,355,198 B1	3/2002	Kim et al.	6,766,817 B2	7/2004	da Silva
6,357,670 B2	3/2002	Ganan-Calvo	6,767,194 B2	7/2004	Jeon et al.
6,386,463 B1	5/2002	Ganan-Calvo	6,767,704 B2	7/2004	Waldman et al.
6,391,559 B1	5/2002	Brown et al.	6,790,328 B2	9/2004	Jacobson et al.
6,394,429 B2	5/2002	Ganan-Calvo	6,793,753 B2	9/2004	Unger et al.
6,399,339 B1	6/2002	Wolberg et al.	6,797,056 B2	9/2004	David
6,399,389 B1	6/2002	Parce et al.	6,800,849 B2	10/2004	Staats
6,403,373 B1	6/2002	Scanlan et al.	6,806,058 B2	10/2004	Jespersion et al.
6,405,936 B1	6/2002	Ganan-Calvo	6,808,382 B2	10/2004	Lanfranchi
6,408,878 B2	6/2002	Unger et al.	6,808,882 B2	10/2004	Griffiths et al.
6,409,832 B2	6/2002	Weigl et al.	6,814,980 B2	11/2004	Levy et al.
6,429,025 B1	8/2002	Parce et al.	6,818,395 B1	11/2004	Quake et al.
6,429,148 B1	8/2002	Chu et al.	6,832,787 B1	12/2004	Renzi
6,432,143 B2	8/2002	Kubiak et al.	6,833,242 B2	12/2004	Quake et al.
6,432,148 B1	8/2002	Ganan-Calvo	6,841,350 B2	1/2005	Ogden et al.
6,432,630 B1	8/2002	Blankenstein	6,872,250 B2	3/2005	David et al.
6,439,103 B1	8/2002	Miller	6,890,487 B1	5/2005	Sklar et al.
6,440,706 B1	8/2002	Vogelstein et al.	6,897,018 B1	5/2005	Yuan et al.
6,450,139 B1	9/2002	Watanabe	6,905,844 B2	6/2005	Kim
6,450,189 B1	9/2002	Ganan-Calvo	6,918,404 B2	7/2005	Dias da Silva
6,454,193 B1	9/2002	Busick et al.	6,926,313 B1	8/2005	Renzi
6,464,336 B1	10/2002	Sharma	6,935,768 B2	8/2005	Lowe et al.
6,464,886 B2	10/2002	Ganan-Calvo	6,936,417 B2	8/2005	Orntoft
6,475,441 B1	11/2002	Parce et al.	6,942,978 B1	9/2005	O'Brien
6,481,648 B1	11/2002	Zimmermann	6,949,342 B2	9/2005	Golub et al.
6,489,103 B1	12/2002	Griffiths et al.	6,960,437 B2	11/2005	Enzelberger et al.
6,503,933 B1	1/2003	Moloney et al.	6,974,667 B2	12/2005	Horne et al.
6,506,609 B1	1/2003	Wada et al.	6,998,232 B1	2/2006	Feinstein et al.
6,508,988 B1	1/2003	Van Dam et al.	7,022,472 B2	4/2006	Robbins et al.
			7,041,481 B2	5/2006	Anderson et al.
			7,049,072 B2	5/2006	Seshi
			7,056,674 B2	6/2006	Baker et al.
			7,057,026 B2	6/2006	Barnes et al.
			7,066,586 B2	6/2006	da Silva

(56)

References Cited

U.S. PATENT DOCUMENTS

7,068,874 B2	6/2006	Wang et al.	7,691,576 B2	4/2010	Holliger et al.
7,078,180 B2	7/2006	Genetta	7,698,287 B2	4/2010	Becker et al.
7,081,192 B1	7/2006	Wang et al.	7,708,949 B2	5/2010	Stone et al.
7,081,340 B2	7/2006	Baker et al.	7,718,578 B2	5/2010	Griffiths et al.
7,090,983 B1	8/2006	Muramatsu et al.	7,736,890 B2	6/2010	Sia et al.
7,115,230 B2	10/2006	Sundararajan et al.	7,741,130 B2	6/2010	Lee, Jr. et al.
7,118,910 B2	10/2006	Unger et al.	RE41,780 E	9/2010	Anderson et al.
7,129,091 B2	10/2006	Ismagilov et al.	7,814,175 B1	10/2010	Chang et al.
7,138,233 B2	11/2006	Griffiths et al.	7,824,889 B2	11/2010	Vogelstein et al.
7,153,700 B1	12/2006	Pardee et al.	7,888,017 B2	2/2011	Quake et al.
7,156,917 B2	1/2007	Moriyama et al.	7,897,044 B2	3/2011	Hoyos et al.
7,163,801 B2	1/2007	Reed	7,897,341 B2	3/2011	Griffiths et al.
7,169,560 B2	1/2007	Lapidus et al.	7,901,939 B2	3/2011	Ismagliov et al.
7,171,311 B2	1/2007	Dai et al.	7,915,015 B2	3/2011	Vogelstein et al.
7,198,899 B2	4/2007	Schleyer et al.	7,968,287 B2	6/2011	Griffiths et al.
7,204,431 B2	4/2007	Li et al.	7,990,525 B2	8/2011	Kanda
7,229,770 B1	6/2007	Price et al.	8,012,382 B2	9/2011	Kim et al.
7,252,943 B2	8/2007	Griffiths et al.	8,067,159 B2	11/2011	Brown et al.
7,267,938 B2	9/2007	Anderson et al.	8,153,402 B2	4/2012	Holliger et al.
7,268,167 B2	9/2007	Higuchi et al.	8,257,925 B2	9/2012	Brown et al.
7,282,337 B1	10/2007	Harris	8,278,071 B2	10/2012	Brown et al.
7,291,462 B2	11/2007	O'Brien et al.	8,278,711 B2	10/2012	Rao et al.
7,294,503 B2	11/2007	Quake et al.	8,318,434 B2	11/2012	Cuppens
7,300,765 B2	11/2007	Patel	8,337,778 B2	12/2012	Stone et al.
7,308,364 B2	12/2007	Shaughnessy et al.	8,436,993 B2	5/2013	Kaduchak et al.
7,314,721 B2	1/2008	Gure et al.	8,528,589 B2	9/2013	Miller et al.
7,316,906 B2	1/2008	Chiorazzi et al.	8,592,221 B2	11/2013	Fraden et al.
7,326,529 B2	2/2008	Ali et al.	8,673,595 B2	3/2014	Nakamura et al.
7,332,280 B2	2/2008	Levy et al.	8,765,485 B2	7/2014	Link et al.
7,332,590 B2	2/2008	Nacht et al.	8,772,046 B2	7/2014	Fraden et al.
7,341,211 B2	3/2008	Ganan Calvo et al.	2001/0010338 A1	8/2001	Ganan-Calvo
7,348,142 B2	3/2008	Wang	2001/0020011 A1	9/2001	Mathiowitz et al.
7,358,231 B1	4/2008	McCaffey et al.	2001/0023078 A1	9/2001	Bawendi et al.
7,361,474 B2	4/2008	Siegler	2001/0029983 A1	10/2001	Unger et al.
7,364,862 B2	4/2008	Ali et al.	2001/0034025 A1*	10/2001	Modlin et al. 435/6
7,368,255 B2	5/2008	Bae et al.	2001/0034031 A1	10/2001	Short et al.
7,378,233 B2	5/2008	Sidransky et al.	2001/0041343 A1	11/2001	Pankowsky
7,378,280 B2	5/2008	Quake et al.	2001/0041344 A1	11/2001	Sepetov et al.
7,390,463 B2	6/2008	He et al.	2001/0041357 A1*	11/2001	Fouillet et al. 435/91.1
7,393,665 B2	7/2008	Brenner	2001/0042793 A1	11/2001	Ganan-Calvo
7,416,851 B2	8/2008	Davi et al.	2001/0048900 A1	12/2001	Bardell et al.
7,429,467 B2	9/2008	Holliger et al.	2001/0050881 A1	12/2001	Depaoli et al.
7,432,064 B2	10/2008	Salceda et al.	2002/0004532 A1	1/2002	Matathia et al.
7,442,507 B2	10/2008	Polsky et al.	2002/0005354 A1	1/2002	Spence et al.
7,449,303 B2	11/2008	Coignet	2002/0008028 A1	1/2002	Jacobson et al.
7,468,271 B2	12/2008	Golovchenko et al.	2002/0012971 A1	1/2002	Mehta
7,473,530 B2	1/2009	Huttemann	2002/0022038 A1	2/2002	Biatry et al.
7,473,531 B1	1/2009	Domon et al.	2002/0022261 A1	2/2002	Anderson et al.
7,476,506 B2	1/2009	Schleyer et al.	2002/0033422 A1	3/2002	Ganan-Calvo
7,479,370 B2	1/2009	Coignet	2002/0036018 A1	3/2002	McNeely et al.
7,479,371 B2	1/2009	Ando et al.	2002/0036139 A1	3/2002	Becker et al.
7,479,376 B2	1/2009	Waldman et al.	2002/0058332 A1	5/2002	Quake et al.
7,482,129 B2	1/2009	Soyupak et al.	2002/0067800 A1	6/2002	Newman et al.
7,501,244 B2	3/2009	Reinhard et al.	2002/0085961 A1	7/2002	Morin et al.
7,504,214 B2	3/2009	Erlander et al.	2002/0119459 A1	8/2002	Griffiths
7,507,532 B2	3/2009	Chang et al.	2002/0127591 A1*	9/2002	Wada et al. 435/6
7,507,541 B2	3/2009	Raitano et al.	2002/0143437 A1	10/2002	Handique et al.
7,510,707 B2	3/2009	Platica et al.	2002/0155080 A1	10/2002	Glenn et al.
7,510,842 B2	3/2009	Podust et al.	2002/0158027 A1	10/2002	Moon et al.
7,514,209 B2	4/2009	Dai et al.	2002/0164271 A1	11/2002	Ho
7,514,210 B2	4/2009	Holliger et al.	2002/0164629 A1	11/2002	Quake et al.
7,524,633 B2	4/2009	Sidransky	2002/0166582 A1	11/2002	O'Connor et al.
7,527,933 B2	5/2009	Sahin et al.	2003/0012586 A1	1/2003	Iwata et al.
7,537,897 B2	5/2009	Brenner et al.	2003/0015425 A1	1/2003	Bohm et al.
7,541,383 B2	6/2009	Fu et al.	2003/0017579 A1	1/2003	Corn et al.
7,544,473 B2	6/2009	Brenner	2003/0039169 A1	2/2003	Ehrfeld et al.
7,556,776 B2	7/2009	Fraden et al.	2003/0059764 A1	3/2003	Ravkin et al.
7,582,446 B2	9/2009	Griffiths et al.	2003/0061687 A1	4/2003	Hansen et al.
7,622,081 B2	11/2009	Chou et al.	2003/0064414 A1	4/2003	Benecky et al.
7,632,562 B2	12/2009	Nair et al.	2003/0082795 A1	5/2003	Shuler et al.
7,635,562 B2	12/2009	Harris et al.	2003/0124586 A1	7/2003	Griffiths et al.
7,638,276 B2	12/2009	Griffiths et al.	2003/0144260 A1	7/2003	Gilon
7,655,435 B2	2/2010	Holliger et al.	2003/0148544 A1	8/2003	Nie et al.
7,655,470 B2	2/2010	Ismagilov et al.	2003/0181574 A1	9/2003	Adam et al.
7,666,593 B2	2/2010	Lapidus	2003/0183525 A1	10/2003	Elrod et al.
			2003/0207295 A1	11/2003	Gunderson et al.
			2003/0219754 A1*	11/2003	Oleksy et al. 435/6
			2003/0224509 A1	12/2003	Moon et al.
			2003/0229376 A1	12/2003	Sandhu

(56)

References Cited

U.S. PATENT DOCUMENTS

2003/0230486	A1	12/2003	Chien et al.	2006/0094119	A1	5/2006	Ismagilov et al.
2003/0232356	A1	12/2003	Dooley et al.	2006/0108012	A1	5/2006	Barrow et al.
2004/0005582	A1	1/2004	Shipwash	2006/0110759	A1	5/2006	Paris et al.
2004/0005594	A1	1/2004	Holliger et al.	2006/0115821	A1	6/2006	Einstein et al.
2004/0018525	A1	1/2004	Wirtz et al.	2006/0147909	A1	7/2006	Rarbach et al.
2004/0027915	A1	2/2004	Lowe et al.	2006/0153924	A1	7/2006	Griffiths et al.
2004/0031688	A1	2/2004	Shenderov	2006/0154298	A1	7/2006	Griffiths et al.
2004/0037813	A1	2/2004	Simpson et al.	2006/0160762	A1	7/2006	Zetter et al.
2004/0041093	A1	3/2004	Schultz et al.	2006/0163385	A1	7/2006	Link et al.
2004/0050946	A1	3/2004	Wang et al.	2006/0169800	A1	8/2006	Rosell et al.
2004/0053247	A1	3/2004	Cordon-Cardo et al.	2006/0177832	A1	8/2006	Brenner
2004/0068019	A1	4/2004	Higuchi et al.	2006/0195269	A1	8/2006	Yeatman et al.
2004/0071781	A1	4/2004	Chattopadhyay et al.	2006/0223127	A1	10/2006	Yip et al.
2004/0079881	A1	4/2004	Fischer et al.	2006/0234254	A1	10/2006	An et al.
2004/0086892	A1	5/2004	Crothers et al.	2006/0234259	A1	10/2006	Rubin et al.
2004/0096515	A1	5/2004	Bausch et al.	2006/0252057	A1	11/2006	Raponi et al.
2004/0134854	A1	7/2004	Higuchi et al.	2006/0257893	A1*	11/2006	Takahashi et al. 435/6
2004/0136497	A1	7/2004	Meldrum et al.	2006/0258841	A1	11/2006	Michl et al.
2004/0146921	A1	7/2004	Eveleigh et al.	2006/0263888	A1	11/2006	Fritz et al.
2004/0159633	A1	8/2004	Whitesides et al.	2006/0269558	A1	11/2006	Murphy et al.
2004/0181131	A1	9/2004	Maynard et al.	2006/0269971	A1	11/2006	Diamandis
2004/0181343	A1	9/2004	Wigstrom et al.	2006/0281089	A1	12/2006	Gibson et al.
2004/0182712	A1	9/2004	Basol	2007/0003442	A1	1/2007	Link et al.
2004/0188254	A1	9/2004	Spaid	2007/0026439	A1	2/2007	Faulstich et al.
2004/0224419	A1	11/2004	Zheng et al.	2007/0045117	A1	3/2007	Pamula et al.
2004/0241693	A1	12/2004	Ricoul et al.	2007/0048744	A1	3/2007	Lapidus
2004/0253731	A1	12/2004	Holliger et al.	2007/0053896	A1	3/2007	Ahmed et al.
2004/0258203	A1	12/2004	Yamano et al.	2007/0054119	A1	3/2007	Garstecki et al.
2004/0259083	A1	12/2004	Oshima	2007/0056853	A1	3/2007	Aizenberg et al.
2005/0000970	A1	1/2005	Kimbara et al.	2007/0077572	A1	4/2007	Tawfik et al.
2005/0003380	A1	1/2005	Cohen et al.	2007/0077579	A1	4/2007	Griffiths et al.
2005/0019776	A1	1/2005	Callow et al.	2007/0092914	A1	4/2007	Griffiths et al.
2005/0032238	A1	2/2005	Karp et al.	2007/0120899	A1	5/2007	Ohnishi et al.
2005/0032240	A1	2/2005	Lee et al.	2007/0154889	A1	7/2007	Wang
2005/0037392	A1	2/2005	Griffiths et al.	2007/0166705	A1	7/2007	Milton et al.
2005/0042639	A1*	2/2005	Knapp et al. 435/6	2007/0172873	A1	7/2007	Brenner et al.
2005/0042648	A1	2/2005	Griffiths et al.	2007/0184439	A1	8/2007	Guilford et al.
2005/0048467	A1	3/2005	Sastry et al.	2007/0184489	A1	8/2007	Griffiths et al.
2005/0064460	A1	3/2005	Holliger et al.	2007/0195127	A1	8/2007	Ahn et al.
2005/0069920	A1	3/2005	Griffiths et al.	2007/0213410	A1	9/2007	Hastwell et al.
2005/0079510	A1	4/2005	Berka et al.	2007/0243634	A1	10/2007	Pamula et al.
2005/0084923	A1	4/2005	Mueller et al.	2007/0259351	A1	11/2007	Chinitz et al.
2005/0087122	A1	4/2005	Ismagliov et al.	2007/0259368	A1	11/2007	An et al.
2005/0095611	A1	5/2005	Chan et al.	2007/0259374	A1	11/2007	Griffiths et al.
2005/0100895	A1	5/2005	Waldman et al.	2007/0292869	A1	12/2007	Becker et al.
2005/0103690	A1	5/2005	Kawano et al.	2008/0003142	A1	1/2008	Link et al.
2005/0118723	A1*	6/2005	Padmanabhan G01N 15/1404 436/164	2008/0003571	A1	1/2008	McKernan et al.
2005/0129582	A1	6/2005	Breidford et al.	2008/0004436	A1	1/2008	Tawfik et al.
2005/0152908	A1	7/2005	Liew et al.	2008/0009005	A1	1/2008	Kruk
2005/0164239	A1	7/2005	Griffiths et al.	2008/0014589	A1	1/2008	Link et al.
2005/0169797	A1*	8/2005	Oshima 422/50	2008/0014590	A1	1/2008	Dahary et al.
2005/0170373	A1	8/2005	Monforte	2008/0020940	A1	1/2008	Stedrinsky et al.
2005/0170431	A1	8/2005	Ibrahim et al.	2008/0021330	A1	1/2008	Hwang et al.
2005/0172476	A1	8/2005	Stone et al.	2008/0023330	A1	1/2008	Viovy et al.
2005/0183995	A1	8/2005	Deshpande et al.	2008/0038754	A1	2/2008	Farias-Eisner et al.
2005/0202489	A1*	9/2005	Cho et al. 435/6	2008/0044828	A1	2/2008	Kwok
2005/0207940	A1	9/2005	Butler et al.	2008/0050378	A1	2/2008	Nakamura et al.
2005/0208495	A1*	9/2005	Joseph et al. 435/6	2008/0050723	A1	2/2008	Belacel et al.
2005/0221339	A1	10/2005	Griffiths et al.	2008/0053205	A1	3/2008	Pollack et al.
2005/0226742	A1	10/2005	Unger et al.	2008/0057514	A1	3/2008	Goldenring
2005/0227264	A1*	10/2005	Nobile et al. 435/6	2008/0058432	A1	3/2008	Wang et al.
2005/0248066	A1	11/2005	Esteban	2008/0063227	A1	3/2008	Rohrseitz
2005/0260566	A1	11/2005	Fischer et al.	2008/0064047	A1	3/2008	Zetter et al.
2005/0272159	A1	12/2005	Ismagilov et al.	2008/0081330	A1	4/2008	Kahvejian
2006/0003347	A1	1/2006	Griffiths et al.	2008/0081333	A1	4/2008	Mori et al.
2006/0003429	A1	1/2006	Frost et al.	2008/0092973	A1	4/2008	Lai
2006/0003439	A1	1/2006	Ismagilov et al.	2008/0113340	A1	5/2008	Schlegel
2006/0035386	A1	2/2006	Hattori et al.	2008/0118462	A1	5/2008	Alani et al.
2006/0036348	A1	2/2006	Handique et al.	2008/0124726	A1	5/2008	Monforte
2006/0046257	A1	3/2006	Pollock et al.	2008/0138806	A1	6/2008	Chow et al.
2006/0051329	A1	3/2006	Lee et al.	2008/0166772	A1	7/2008	Hollinger et al.
2006/0068398	A1	3/2006	McMillan	2008/0166793	A1	7/2008	Beer et al.
2006/0078888	A1	4/2006	Griffiths et al.	2008/0171078	A1	7/2008	Gray
2006/0078893	A1	4/2006	Griffiths et al.	2008/0176211	A1	7/2008	Spence et al.
				2008/0176236	A1	7/2008	Tsao et al.
				2008/0181850	A1	7/2008	Thaxton et al.
				2008/0206756	A1	8/2008	Lee et al.
				2008/0220986	A1	9/2008	Gormley et al.
				2008/0222741	A1	9/2008	Chinnaiyan

(56)

References Cited

U.S. PATENT DOCUMENTS

2008/0234138 A1 9/2008 Shaughnessy et al.
 2008/0234139 A1 9/2008 Shaughnessy et al.
 2008/0268473 A1 10/2008 Moses et al.
 2008/0269157 A1 10/2008 Srivastava et al.
 2008/0274513 A1* 11/2008 Shenderov et al. 435/91.2
 2008/0274908 A1 11/2008 Chang
 2008/0280302 A1 11/2008 Kebebew
 2008/0286199 A1 11/2008 Livingston et al.
 2008/0286801 A1 11/2008 Arjol et al.
 2008/0286811 A1 11/2008 Moses et al.
 2008/0293578 A1 11/2008 Shaughnessy et al.
 2008/0299565 A1* 12/2008 Schneider et al. 435/6
 2008/0311570 A1 12/2008 Lai
 2008/0311604 A1 12/2008 Elting et al.
 2009/0004687 A1 1/2009 Mansfield et al.
 2009/0005254 A1 1/2009 Griffiths et al.
 2009/0012187 A1 1/2009 Chu et al.
 2009/0017463 A1 1/2009 Bhowmick
 2009/0021728 A1 1/2009 Heinz et al.
 2009/0023137 A1 1/2009 Van Der Zee et al.
 2009/0026082 A1 1/2009 Rothberg et al.
 2009/0029372 A1 1/2009 Wewer
 2009/0042737 A1 2/2009 Katz et al.
 2009/0053700 A1 2/2009 Griffiths et al.
 2009/0053732 A1 2/2009 Vermesh et al.
 2009/0060797 A1 3/2009 Mathies et al.
 2009/0062144 A1 3/2009 Guo
 2009/0068170 A1 3/2009 Weitz et al.
 2009/0075265 A1 3/2009 Budiman et al.
 2009/0075307 A1 3/2009 Fischer et al.
 2009/0075311 A1 3/2009 Karl
 2009/0081237 A1 3/2009 D'Andrea et al.
 2009/0081685 A1 3/2009 Beyer et al.
 2009/0087849 A1 4/2009 Malinowski et al.
 2009/0092973 A1 4/2009 Erlander et al.
 2009/0098542 A1 4/2009 Budiman et al.
 2009/0098543 A1 4/2009 Budiman et al.
 2009/0105959 A1 4/2009 Braverman et al.
 2009/0118128 A1 5/2009 Liu et al.
 2009/0124569 A1 5/2009 Bergan et al.
 2009/0127454 A1 5/2009 Ritchie et al.
 2009/0127589 A1 5/2009 Rothberg et al.
 2009/0131353 A1 5/2009 Insel et al.
 2009/0131543 A1 5/2009 Weitz et al.
 2009/0191565 A1 7/2009 Lapidus et al.
 2009/0197248 A1 8/2009 Griffiths et al.
 2009/0197772 A1 8/2009 Griffiths et al.
 2009/0226972 A1 9/2009 Beer et al.
 2009/0233802 A1 9/2009 Bignell et al.
 2009/0246788 A1 10/2009 Albert et al.
 2009/0325236 A1 12/2009 Griffiths et al.
 2010/0003687 A1 1/2010 Simen et al.
 2010/0009353 A1 1/2010 Barnes et al.
 2010/0022414 A1 1/2010 Link et al.
 2010/0035252 A1 2/2010 Rothberg et al.
 2010/0075436 A1 3/2010 Urdea et al.
 2010/0105112 A1 4/2010 Holtze et al.
 2010/0111768 A1 5/2010 Banerjee et al.
 2010/0124759 A1 5/2010 Wang et al.
 2010/0130369 A1 5/2010 Shenderov et al.
 2010/0136544 A1 6/2010 Agresti et al.
 2010/0137143 A1 6/2010 Rothberg et al.
 2010/0137163 A1 6/2010 Link et al.
 2010/0159592 A1 6/2010 Holliger et al.
 2010/0172803 A1 7/2010 Stone et al.
 2010/0173394 A1 7/2010 Colston, Jr. et al.
 2010/0188073 A1 7/2010 Rothberg et al.
 2010/0197507 A1 8/2010 Rothberg et al.
 2010/0210479 A1 8/2010 Griffiths et al.
 2010/0213628 A1 8/2010 Bausch et al.
 2010/0233026 A1 9/2010 Ismagliov et al.
 2010/0282617 A1 11/2010 Rothberg et al.
 2010/0300559 A1 12/2010 Schultz et al.
 2010/0300895 A1 12/2010 Nobile et al.
 2010/0301398 A1 12/2010 Rothberg et al.

2010/0304982 A1 12/2010 Hinz et al.
 2011/0000560 A1 1/2011 Miller et al.
 2011/0024455 A1 2/2011 Bethuy et al.
 2011/0033854 A1 2/2011 Drmanac et al.
 2011/0053151 A1 3/2011 Hansen et al.
 2011/0142734 A1 6/2011 Ismagliov et al.
 2011/0174622 A1 7/2011 Ismagilov et al.
 2011/0176966 A1 7/2011 Ismagilov et al.
 2011/0177494 A1 7/2011 Ismagilov et al.
 2011/0177586 A1 7/2011 Ismagilov et al.
 2011/0177609 A1 7/2011 Ismagilov et al.
 2011/0188717 A1 8/2011 Baudry et al.
 2011/0190146 A1 8/2011 Boehm et al.
 2011/0244455 A1 10/2011 Larson et al.
 2011/0250597 A1 10/2011 Larson et al.
 2011/0275063 A1 11/2011 Weitz et al.
 2012/0010098 A1 1/2012 Griffiths et al.
 2012/0015382 A1 1/2012 Weitz et al.
 2012/0015822 A1 1/2012 Weitz et al.
 2013/0157872 A1 6/2013 Griffiths et al.
 2013/0178368 A1 7/2013 Griffiths et al.
 2013/0217601 A1 8/2013 Griffiths et al.
 2013/0295568 A1 11/2013 Link

FOREIGN PATENT DOCUMENTS

AU 680195 B2 7/1997
 AU 1276099 A 6/1999
 AU 747464 B2 5/2002
 AU 768399 B2 12/2003
 AU 2010224352 A1 10/2010
 BR 8200642 A 12/1982
 BR 9710052 A 1/2000
 CA 1093344 A1 1/1981
 CH 563 087 A5 6/1975
 DE 2100685 A1 7/1972
 DE 3042915 A1 9/1981
 DE 43 08 839 C2 4/1997
 DE 69126763 T2 2/1998
 DE 199 61 257 A1 7/2001
 DE 100 15 109 A1 10/2001
 DE 100 41 823 A1 3/2002
 EP 0047130 B1 2/1985
 EP 0402995 A2 12/1990
 EP 0249007 A3 3/1991
 EP 0418635 A1 3/1991
 EP 0476178 A1 3/1992
 EP 0618001 10/1994
 EP 0718038 A2 6/1996
 EP 0540281 B1 7/1996
 EP 0528580 B1 12/1996
 EP 0486351 B1 7/1997
 EP 0895120 2/1999
 EP 1362634 A1 11/2003
 EP 1741482 1/2007
 EP 2127736 12/2009
 ES 2 095 413 T3 2/1997
 FR 2 404 834 A1 4/1979
 FR 2 451 579 A1 10/1980
 FR 2 469 714 A1 5/1981
 FR 2 470 385 A1 5/1981
 FR 2 650 657 A1 2/1991
 FR 2 669 028 A1 5/1992
 FR 2 703 263 A1 10/1994
 GB 1148543 4/1969
 GB 1 446 998 8/1976
 GB 2 005 224 4/1979
 GB 2 047 880 12/1980
 GB 2 062 225 5/1981
 GB 2 064 114 6/1981
 GB 2 097 692 A 11/1982
 GB 2 210 532 6/1989
 IE 922432 A1 2/1993
 JP S5372016 A 6/1978
 JP S5455495 A 5/1979
 JP 55125472 9/1980
 JP S5636053 A 4/1981
 JP 56-124052 9/1981
 JP 59-49832 A 3/1984

(56)

References Cited

FOREIGN PATENT DOCUMENTS			WO		
			WO	00/47322	2/2000
			WO	00/52455	2/2000
			WO	00/40712	6/2000
			WO	00/54735	9/2000
			WO	00/61275	10/2000
			WO	00/70080	11/2000
			WO	00/76673	12/2000
			WO	00/078455 A1	12/2000
			WO	01/12327	2/2001
			WO	01/14589	3/2001
			WO	01/18244	3/2001
			WO	01/64332	9/2001
			WO	01/68257	9/2001
			WO	01/69289	9/2001
			WO	01/72431	10/2001
			WO	01/80283	10/2001
			WO	01/89787 A2	11/2001
			WO	01/89788 A2	11/2001
			WO	01/94635 A2	12/2001
			WO	02/16017	2/2002
			WO	02/18949	3/2002
			WO	02/22869	3/2002
			WO	02/23163	3/2002
			WO	02/31203	4/2002
			WO	02/047665	8/2002
			WO	02/060275	8/2002
			WO	02/060591 A1	8/2002
			WO	02/068104 A1	9/2002
			WO	02/078845	10/2002
			WO	02/103011	12/2002
			WO	02/103363	12/2002
			WO	03/011443	2/2003
			WO	03/026798 A1	4/2003
			WO	03/037302	5/2003
			WO	03/044187	5/2003
			WO	03/078659	9/2003
			WO	03/099843	12/2003
			WO	2004/002627	1/2004
			WO	2004/018497	3/2004
			WO	2004/024917	3/2004
			WO	2004/037374 A2	5/2004
			WO	2004/038363	5/2004
			WO	2004/069849	8/2004
			WO	2004/071638 A2	8/2004
			WO	2004/074504	9/2004
			WO	2004/083443	9/2004
			WO	2004/087308	10/2004
			WO	2004/088314	10/2004
			WO	2004/091763	10/2004
			WO	2004/102204	11/2004
			WO	2004/103565	12/2004
			WO	2005/000970	1/2005
			WO	2005/002730	1/2005
			WO	2005/003375 A2	1/2005
			WO	2005/021151	3/2005
			WO	2005/023427 A1	3/2005
			WO	2005/049787 A2	6/2005
			WO	2005/103106	11/2005
			WO	2005/118138	12/2005
			WO	2005/118867 A2	12/2005
			WO	2006/002641	1/2006
			WO	2006/009657	1/2006
			WO	2006/027757	3/2006
			WO	2006/038035	4/2006
			WO	2006/040551	4/2006
			WO	2006/040554	4/2006
			WO	2006/078841	7/2006
			WO	2006/096571	9/2006
			WO	2006/101851	9/2006
			WO	2007/021343	2/2007
			WO	2007/030501	3/2007
			WO	2007/081385	7/2007
			WO	2007/081387	7/2007
			WO	2007/089541	8/2007
			WO	2007/114794	10/2007
			WO	2007/123744	11/2007
			WO	2007/133710	11/2007
			WO	2007/138178	12/2007
			WO	2008/021123	2/2008

(56)

References Cited

FOREIGN PATENT DOCUMENTS

WO	2008/063227	5/2008
WO	2008/097559	8/2008
WO	2008/115626 A2	9/2008
WO	2008/121342	10/2008
WO	2008/130623	10/2008
WO	2008/134153 A1	11/2008
WO	2009/015296 A1	1/2009
WO	2009/029229	3/2009
WO	2009/085929 A1	7/2009
WO	2010/056728	5/2010
WO	2010/040006	8/2010
WO	2010/151776	12/2010
WO	2011/042564	4/2011
WO	2011/079176	6/2011
WO	2012/022976 A1	2/2012
WO	2012/048341 A1	4/2012

OTHER PUBLICATIONS

- International Search Report in PCT/US01/18400 Mailed Jan. 28, 2005 (37 pages).
- International Search Report in PCT/US01/18400 Mailed Jan. 28, 2005 (37 pages).
- Ismagilov, Integrated Microfluidic Systems, *Angew. Chem. Int. Ed* 42:4130-4132 (2003).
- ISR and Written Opinion for PCT/US2013/037751 dated Aug. 22, 2013 (16 pages).
- Janda, et al, Chemical selection for catalysis in combinatorial antibody libraries, *Science*, 275:945-948 (1997).
- Jang et al., Controllable delivery of non-viral DNA from porous scaffold, *J Controlled Release* 86(1):157-168 (2003).
- Japanese Notice of Reasons for Rejection for JP 2006-509830 mailed Jun. 1, 2011 (4 pages).
- Japanese Office Action for JP 2006-509830 mailed Jun. 1, 2011 (4 pages).
- Jermutus et al., Recent advances in producing and selecting functional proteins by using cell-free translation, *Curr Opin Biotechnol* 9(5): 534-48 (1998).
- Jestin et al., A Method for the Selection of Catalytic Activity Using Phage Display and Proximity Coupling, *Agnew. Chem. Int. Ed. Engi.* 38(8):1124-1127 (1999).
- Jo, et al, Encapsulation of Bovine Serum Albumin in Temperature-Programmed Shell-in-Shell Structures, *Macromol. Rapid Comm* 24:957-962 (2003).
- Joerger et al., Analyte detection with DNA-labeled antibodies and polymerase chain reaction, *Clin. Chem.* 41(9):1371-7 (1995).
- Johannsson et al., Amplification by Second Enzymes, In *ELISA and Other Solid Phase Immunoassays*, Kemeny et al (ed.), Chapter 4, pp. 85-106 John Wiley (1988).
- Johannsson, A., Heterogeneous Enzyme Immunoassays, In *Principles and Practice of Immunoassay*, pp. 295-325 Stockton Press (1991).
- Johnson, T.O. et al., Protein tyrosine phosphatase 1B inhibitors for diabetes, *Nature Review Drug Discovery* 1, 696-709 (2002).
- Jones et al. Glowing jellyfish, luminescence and a molecule called coelenterazine, *Trends Biotechnol.* 17(12):477-81 (1999).
- Jones, L.J. et al., Quenched BODIPY dye-labeled casein substrates for the assay of protease activity by direct fluorescence measurement, *Anal Biochem*, 251:144 (1997).
- Joo et al., Laboratory evolution of peroxide-mediated cytochrome P450 hydroxylase, *Nature* 399:670 (1999).
- Joos et al., Covalent attachment of hybridizable oligonucleotides to glass supports, *Analytical Biochemistry* 247:96-101 (1997).
- Joyce, G.F., In vitro Evolution of Nucleic Acids, *Curr. Opp. Structural Biol*, 4: 331-336 (1994).
- Kadir and Moore, Haem binding to horse spleen ferritin, *Febs Lett*, 276: 81-4 (1990).
- Kallen, R.G. et al., The mechanism of the condensation of formaldehyde with tetrahydrofolic acid, *J. Biol. Chem.*, 241:5851-63 (1966).
- Kambara et al., Optimization of Parameters in a DNA Sequenator Using Fluorescence Detection, *Nature Biotechnology* 6:816-821 (1988).
- Kamensky et al., Spectrophotometer: new instrument for ultrarapid cell analysis, *Science* 150(3696):630-631 (1965).
- Kanouni et al., Preparation of a stable double emulsion (W1/O/W2): role of the interfacial films on the stability of the system, *Adv. Cond. Interf. Sci.*, 99(3): 229-254 (2002).
- Katanaev et al., Viral Q beta RNA as a high expression vector for mRNA translation in a cell-free system, *Febs Lett*, 359:89-92 (1995).
- Katsura et al., Indirect micromanipulation of single molecules in water-in-oil emulsion, *Electrophoresis*, 22:289-93 (2001).
- Kawakatsu et al., Regular-sized cell creation in microchannel emulsification by visual microprocessing method, *Journal of the American Oil Chemists Society*, 74:317-21 (1997).
- Keana J. & Cai, S. X., New reagents for photoaffinity labeling: synthesis and photolysis of functionalized perfluorophenyl azides, *J. Org. Chem.*55(11):3640-3647 (1990).
- Keefe, A.D. et al., Functional proteins from a random-sequence library, *Nature*, 410: 715-718 (2001).
- Keij et al., High-Speed Photodamage Cell Selection Using a Frequency-Doubled Argon Ion Laser, *Cytometry*, 19(3): 209-216 (1995).
- Keij, J.F., et al., High-speed photodamage cell sorting: An evaluation of the Zapper prototype, *Methods in cell biology*, 42: 371-358 (1994).
- Kelly et al., Miniaturizing chemistry and biology in microdroplets, *Chem Commun* 18:1773-1788 (2007).
- Kerker, M., Elastic and inelastic light scattering in flow cytometry, *Cytometry*, 4:1-10 (1983).
- Khandjian, UV crosslinking of RNA to nylon membrane enhances hybridization signals, *Mol. Bio. Rep.* 11: 107-115 (1986).
- Kim et al., Comparative study on sustained release of human growth hormone from semi-crystalline poly(L-lactic acid) and amorphous poly(D,L-lactic-co-glycolic acid) microspheres: morphological effect on protein release, *Journal of Controlled Release*, 98(1):115-125 (2004).
- Kim S. et al, Type II quantum dots: CdTe/CdSe (core/shell) and CdSe/ZnTe (core/shell) heterostructures, *J. Am Chem Soc.* 125:11466-11467 (2003).
- Kircher et al., High-throughput DNA sequencing—concepts and limitations, *Bioessays* 32(6):524-536 (2010).
- Kiss et al., High-throughput quantitative polymerase chain reaction in picoliter droplets, *Anal. Chem* 80:8975-8981 (2008).
- Kitagawa et al., Manipulation of a single cell with microcapillary tubing based on its electrophoretic mobility, *Electrophoresis* 16:1364-1368 (1995).
- Klug and Famulok, All you wanted to know about selex, *Molecular Biology Reports*, 20:97-107 (1994).
- Klug and Schwabe, Protein motifs 5. Zinc fingers, *FASEB J* 9(8):597-604 (1995).
- Klug, A., Gene Regulatory Proteins and Their Interaction with DNA, *Ann NY Acad Sci*, 758: 143-60 (1995).
- Knaak et al., Development of partition coefficients, Vmax and Km values, and allometric relationships, *Toxicol Lett.* 79 (I-3):87-98 (1995).
- Knight, James B., Hydrodynamic Focusing on a Silicon Chip: Mixing Nanoliters in Microseconds, *Physical Review Lett* 80(17):3863-3866 (1998).
- Kojima et al. PCR amplification from single DNA molecules on magnetic beads in emulsion: application for high-throughput screening of transcription factor targets. *Nucleic Acids Res.* 33:e150 (2005).
- Kolb et al., Cotranslational folding of proteins, *Biochem Cell Biol*, 73:1217-20 (1995).
- Komatsu et al., Roles of cytochromes P450 1A2, 2A6, and 2C8 in 5-fluorouracil formation from tegafur, an anticancer prodrug, in human liver microsomes. *Drug Met. Disp.*, 28:1457-1463 (2001).
- Kopp et al., Chemical amplification: continuous flow PCR on a chip, *Science*, 280:1046-48 (1998).
- Koster et al., Drop-based microfluidic devices for encapsulation of single cells, *Lab on a Chip* 8:1110-1115 (2008).

(56)

References Cited

OTHER PUBLICATIONS

- Kowalczykowski et al., Biochemistry of homologous recombination in *Escherichia coli*, *Microbiol Rev* 58(3):401-65 (1994).
- Krafft et al., Emulsions and microemulsions with a fluorocarbon phase, *Colloid and Interface Science* 8(3):251-258 (2003).
- Krafft et al., Synthesis and preliminary data on the biocompatibility and emulsifying properties of perfluoroalkylated phosphoramidates as injectable surfactants, *Eur. J. Med. Chem.*, 26:545-550 (1991).
- Krafft, Fluorocarbons and fluorinated amphiphiles in drug delivery and biomedical research, *Adv Rev Drug Disc* 47:209-228 (2001).
- Kralj et al., Surfactant-enhanced liquid-liquid extraction in microfluidic channels with inline electric-field enhanced coalescence, *Lab Chip* 5:531-535 (2005).
- Krebber, C, et al., Selectivity-infective phage (SIP): a mechanistic dissection of a novel in vivo selection for protein-ligand interactions, *Journal of Molecular Biology*, 268, 607-618 (1997).
- Kricka and Wilding, Microchip PCR, *Anal Bioanal Chem* 377(5):820-825 (2003).
- Kricka and Wilding, Micromachining: a new direction for clinical analyzers, *Pure and Applied Chemistry* 68 (10):1831-1836 (1996).
- Krumdiek, C.L. et al., Solid-phase synthesis of pteroylpolyglutamates, *Methods Enzymol*, 524-29 (1980).
- Kumar, A. et al., Activity and kinetic characteristics of glutathione reductase in vitro in reverse micellar waterpool, *Biochem Biophys Acta*, 996(1-2):1-6 (1989).
- Lage et al., Whole genome analysis of genetic alterations in small DNA samples using hyperbranched strand displacement amplification and array—CGH. *Genome Res.* 13: 294-307 (2003).
- Lamprecht et al., pH-sensitive microsphere delivery increases oral bioavailability of calcitonin, *Journal of Controlled Release*, 98(1): 1-9(2004).
- Lancet, D. et al., Probability model for molecular recognition in biological receptor repertoires: significance to the olfactory system, *PNAS*, 90(8):3715-9 (1993).
- Landergren et al., A ligase mediated gene detection technique. *Science* 241(4869):1077-80 (1988).
- Langmuir, *Directing Droplets Using Microstructured Surfaces*, vol. 22 No. 14, Jun. 9, 2006 p. 6161-6167.
- Lasheras, et al., Breakup and Atomization of a Round Water Jet by a High Speed Annular Air Jet, *J Fluid Mechanics* 357:351-379 (1998).
- Leary et al., Application of Advanced Cytometric and Molecular Technologies to Minimal Residual Disease Monitoring, *Proceedings of SPIE* 3913:36-44 (2000).
- Lee et al, Investigating the target recognition of DNA cytosine-5 methyltransferase HhaI by library selection using in vitro compartmentalisation (IVC), *Nucleic Acids Res* 30:4937-4944 (2002).
- Lee et al., Circulating flows inside a drop under time-periodic non-uniform electric fields, *Phys Fluids* 12(8):1899-1910 (2000).
- Lee, et al, Effective Formation of Silicone-in-Fluorocarbon-in-Water Double Emulsions: Studies on Droplet Morphology and Stability, *Journal of Dispersion Sci Tech* 23(4):491-497(2002).
- Lee, et al, Preparation of Silica Particles Encapsulating Retinol Using O/W/O Multiple Emulsions, *Journal of Colloid and Interface Science*, 240(1): 83-89 (2001).
- Lemof, et al, An AC Magnetohydrodynamic Microfluidic Switch for Micro Total Analysis Systems, *Biomedical Microdevices*, 5(1):55-60 (2003).
- Lesley et al., Use of in vitro protein synthesis from PCR-generated templates to study interaction of *E coli* transcription factors with core RNA polymerase, *J Biol Chem* 266(4):2632-8 (1991).
- Lesley, S.A., Preparation and use of *E. coli* S-30 extracts, *Methods Mol Biol*, 37:265-78 (1995).
- Leung et al., A method for random mutagenesis of a defined DNA segment using a modified polymerase chain reaction. *Technique* 1:11-15 (1989).
- Li and Harrison, Transport, Manipulation, and Reaction of Biological Cells On-Chip Using Electrokinetic Effects, *Analytical Chemistry* 69(8):1564-1568 (1997).
- Li et al., Nanoliter microfluidic hybrid method for simultaneous screening and optimization validated with crystallization of membrane proteins, *PNAS* 103: 19243-19248 (2006).
- Li et al., Single-step procedure for labeling DNA strand breaks with fluorescein-or BODIPY-conjugated deoxynucleotides: detection of apoptosis and bromodeoxyuridine incorporation. *Cytometry* 20:172-180 (1995).
- Liao et al., Isolation of a thermostable enzyme variant by cloning and selection in a thermophile, *PNAS* 83:576-80 (1986).
- Lim et al., Microencapsulated islets as bioartificial endocrine pancreas, *Science* 210(4472):908-10 (1980).
- Lin et al., Self-Assembled Combinatorial Encoding Nanoarrays for Multiplexed Biosensing, *Nanoletter*, 2007, vol. No. 2 p. 507-512.
- Link et al, Geometrically Mediated Breakup of Drops in Microfluidic Devices, *Phys. Rev. Lett.*, 92(5): 054503-1 thru 054503-4 (2004).
- Link et al., Electric control droplets in microfluidic devices, *Angew Chem Int Ed* 45:2556-2560 (2006).
- Lipinski et al., Experimental and Computational Approaches to Estimate Solubility and Permeability in Drug Discovery and Development Settings, *Adv. Drug Deliv. Rev.*, 46:3-26 (2001).
- Lipkin et al., Biomarkers of increased susceptibility to gastrointestinal cancer: new application to studies of cancer prevention in human subjects, *Cancer Research* 48:235-245 (1988).
- Liu et al., Fabrication and characterization of hydrogel-based microvalves, *Mecoelectromech. Syst.*11:45-53 (2002).
- Liu et al., Passive Mixing in a Three-Dimensional Serpentine MicroChannel, *J MEMS* 9(2):190-197 (2000).
- Lizardi et al., Mutation detection and single-molecule counting using isothermal rolling-circle amplification. *Nat Genet* 19(3):225-32 (1998).
- Loakes and Brown, 5-Nitroindole as a universal base analogue. *Nucleic Acids Res* 22: 4039-4043 (1994).
- Loakes et al., Stability and structure of DNA oligonucleotides containing non-specific base analogues. *J. Mol. Biol* 270:426-435 (1997).
- Loeker et al., *Colloids and Surfaces A: Physicochem. Eng. Aspects* 214:143-150, (2003).
- Loeker et al., FTIR analysis of water in supercritical carbon dioxide microemulsions using monofunctional perfluoropolyether surfactants, *Colloids and Surfaces A: Physicochem. Eng. Aspects* 214:143-150, (2003).
- Lopez-Herrera, et al, Coaxial jets generated from electrified Taylor cones. Scaling laws, *Aerosol Science*, 34:535-552 (2003).
- Lopez-Herrera, et al, One-Dimensional Simulation of the Breakup of Capillary Jets of Conducting Liquids Application to E.H.D. Spraying, *Aerosol. Set*, 30 (7): 895-912 (1999).
- Lopez-Herrera, et al, The electrospaying of viscous and non-viscous semi-insulating liquids. Scaling laws, *Bulletin of the American Physical Society*,40 (12):2041(1995).
- Lorenceau et al, Generation of Polymerosomes from Double-Emulsions, *Langmuir*, 21(20): 9183-9186 (2005).
- Lorenz et al, Isolation and expression of a cDNA encoding Renilla reniformis luciferase, *PNAS* 88(10):4438-42 (1991).
- Loscertales, et al, Micro/Nano Encapsulation via Electrified Coaxial Liquid Jets, *Science*, 295(5560): 1695-1698 (2002).
- Low N.M. et al., Mimicking somatic hypermutation: affinity maturation of antibodies displayed on bacteriophage using a bacteriophage mutator strain. *J Mol Biol* 260(3), 359-68 (1996).
- Lowe, K.C., Perfluorochemical respiratory gas carriers: benefits to cell culture systems, *J Fluorine Chem* 118:19-26 (2002).
- Lowman et al., Selecting high affinity binding proteins by monovalent phage display, *Biochemistry* 30(45):10832-8 (1991).
- Lu et al., Robust fluorescein-doped silica nanoparticles via dense-liquid treatment, *Colloids and Surfaces a Physicochemical and Engineering Aspects*, 303(3):207-210 (2007).
- Luisi et al, Activity and Conformation of Enzymes in Reverse Micellar Solutions, *Meth. Enzymol* 136:188-216 (1987).
- Lund et al., Assessment of methods for covalent binding of nucleic acids to magnetic beads, Dynabeads, and the characteristics of the bound nucleic acids in hybridization reactions, *Nucleic Acids Research*, Oxford University Press, 16(22) (1998).

(56)

References Cited

OTHER PUBLICATIONS

- Lunderberg et al., Solid-phase technology: magnetic beads to improve nucleic acid detection and analysis, *Biotechnology Annual Review*, 1:373-401 (1995).
- Lundstrom, et al, Breakthrough in cancer therapy: Encapsulation of drugs and viruses, www.currentdrugdiscovery.com, Nov. 19-23, 2002.
- Lyne, P.D., Structure-Based Virtual Screening: An Overview, *Drug Discov. Today*, 7(20):1047-1055 (2002).
- Ma, C. et al., In vitro protein engineering using synthetic tRNA(Ala) with different anticodons, *Biochemistry* 32 (31):7939-45 (1993).
- Machine translation of JP 2002-282682 (26 pages).
- Mackenzie et al., The application of flow microfluorimetry to biomedical research and diagnosis: a review, *Dev Biol Stand* 64:181-193 (1986).
- Mackenzie, IABS Symposium on Reduction of Animal Usage in the Development and Control of Biological Products, London, UK, 1985.
- Maclean, D. et al., Glossary of terms used in combinatorial chemistry, *Pure Appl. Chem.* 71(12):2349-2365 (1999).
- Magdassi et al., Multiple Emulsions: HLB Shift Caused by Emulsifier Migration to External Interface, *J. Colloid Interface Sci* 97:374-379 (1984).
- Mahajan et al., Bcl-2 and Bax Interactions in Mitochondria Probed with Green Florescent Protein and Fluorescence Resonance Energy Transfer, *Nat. Biotechnol.* 16(6): 547-552 (1998).
- Mahjoob et al., Rapid microfluidic thermal cyler for polymerase chain reaction nucleic acid amplification. *Int J HeatMass Transfer* 2008;51:2109-22.
- Malmborg, A, et al., Selective phage infection mediated by epitope expression on F pilus, *Journal of Molecular Biology*, 273, 544-551 (1997).
- Mammal Wikipedia.com accessed Sep. 22, 2011).
- Manley et al., In vitro transcription: whole cell extract, *Methods Enzymol*, 101:568-82 (1983).
- Manz et al., Micromachining of monocrystalline silicon and glass for chemical analysis systems a look into next century's technology or just a fashionable craze, *Trends in Analytical Chemistry* 10(5):144-149 (1991).
- Mao et al., Kinetic behaviour of alpha-chymotrypsin in reverse micelles: a stopped-flow study, *Eur J Biochem* 208 (1):165-70 (1992).
- Mao, Q. et al., Substrate effects on the enzymatic activity of alphachymotrypsin in reverse micelles, *Biochem Biophys Res Commun*, 178(3):1105-12 (1991).
- Mardis, E.R., The impact of next-generation sequencing technology on genetics, *Trends Genet* 24:133-141 (2008).
- Margulies, M et al., Genome sequencing in microfabricated high-density picolitre reactors, *Nature* 437(7057):376-380 (2005).
- Marques et al., Porous Flow within Concentric Cylinders, *Bull Am Phys Soc Div Fluid Dyn* 41:1768 (1996).
- Mason, T.J. and Bibette, J. Shear Rupturing of Droplets in Complex Fluids, *Langmuir*, 13(17):4600-4613 (1997).
- Mastrobattista et al., High-throughput screening of enzyme libraries: in vitro evolution of a beta-galactosidase by fluorescence-activated sorting of double emulsions, *Chem. Biol.* 12(12): 1291-1300 (2005).
- Masui et al., Probing of DNA-Binding Sites of *Escherichia Coli* RecA Protein Utilizing 1-anilino-naphthalene-8-Sulfonic Acid, *Biochem* 37(35):12133-12143 (1998).
- Matayoshi, E.D. et al., Novel fluorogenic substrates for assaying retroviral proteases by resonance energy transfer, *Science* 247:954 (1990).
- Mattheakis et al., An in vitro polysome display system for identifying ligands from very large peptide libraries, *PNAS* 91:9022-6 (1994).
- Mayr, L.M., and Fuerst, P., The Future of High-Throughput Screening, *JBiomol Screen* 13:443-448 (2008).
- Mazutis et al., Droplet-Based Microfluidic Systems for High-Throughput Single DNA Molecule Isothermal Amplification and Analysis, *Anal Chem* 81(12):4813-4821 (2009).
- Mazutis et al., Multi-step microfluidic droplet processing: kinetic analysis of an in vitro translated enzyme, *Lab Chip* 9:2902-2908 (2009).
- McCafferty et al., Phage antibodies: filamentous phage displaying antibody variable domains, *Nature*, 348: 552-4 (1990).
- McDonald and Whitesides, Poly(dimethylsiloxane) as a material for fabricating microfluidic devices, *Account Chem. Res.* 35:491-499 (2002).
- McDonald et al. Fabrication of microfluidic systems in poly(dimethylsiloxane), *Electrophoresis* 21(1):27-40 (2000).
- Melton et al., Efficient in vitro synthesis of biologically active RNA and RNA hybridization probes from plasmids containing a bacteriophage SP6 promoter, *Nucl. Acids Res.* 12(18):7035-7056 (1984).
- Mendel, D. et al., Site-Directed Mutagenesis with an Expanded Genetic Code, *Annu Rev Biophys Biomol Struct*, 24:435-62 (1995).
- Menger and Yamada, Enzyme catalysis in water pools, *J. Am. Chem. Soc.*, 101:6731-4 (1979).
- Meylan and Howard, Atom/fragment contribution method for estimating octanol-water partition coefficients, *J Pharm Sci.* 84(1):83-92 (1995).
- Miele et al., Autocatalytic replication of a recombinant RNA, *J Mol Biol*, 171:281-95 (1983).
- Minshuil, J. and Stemmer, W.P., Protein evolution by molecular breeding, *Curr Opin Chem Biol* 3(3): 284-90 (1999).
- Miroux and Walker, Over-production of proteins in *Escherichia coli*: mutant hosts that allow synthesis of some membrane proteins and globular proteins at high levels, *J of Mol Biol* 260(3):289-98 (1996).
- Miyawaki et al., Fluorescent Indicators for Ca²⁺ Based on Green Fluorescent Proteins and Calmodulin, *Nature*, 388: 882-887 (1997).
- Mize et al., Dual-enzyme cascade—an amplified method for the detection of alkaline phosphatase, *Anal Biochem* 179 (2): 229-35 (1989).
- Mock et al., A fluorometric assay for the biotin-avidin interaction based on displacement of the fluorescent probe 2-anilino-naphthalene-6-sulfonic acid, *Anal Biochem*, 151:178-81 (1985).
- Moldavan, A., Photo-electric technique for the counting of microscopical cells, *Science* 80:188-189 (1934).
- Montigiani, S. et al., Alanine substitutions in calmodulin-binding peptides result in unexpected affinity enhancement, *J Mol Biol*, 258:6-13 (1996).
- Moore, M.J., Exploration by lamp light, *Nature*, 374:766-7 (1995).
- Moudrianakis and Beer, Base sequence determination in nucleic acids with the electron microscope 3. Chemistry and microscopy of guanine-labeled DNA, *PNAS* 53:564-71 (1965).
- Gasperlin et al., Viscosity prediction of lipophilic semisolid emulsion systems by neural network modeling, *Intl J Pharm*, 196:37-50 (2000).
- Georgiou et al., Display of heterologous proteins on the surface of microorganisms: from the screenign of combinatorial libraires to live recombinant vaccines. *Nat Biotechnol* 15(1), 29-34 (1997).
- Georgiou, G., Analysis of large libraries of protein mutants using flow cytometry, *Adv Protein Chem*, 55: 293-315 (2000).
- Gerdts et al., A Synthetic Reaction NetWork: Chemical Amplification Using Nonequilibrium Autocatalytic Reactions Coupled in Time, *J. Am. Chem. Soc* 126:6327-6331 (2004).
- Ghadessy et al., Directed Evolution of Polymerase Function by Compartmentalized Self-Replication, *PNSAS* 98(8): 4552-4557 (2001).
- Gibbs et al., Detection of single DNA base differences by competitive oligonucleotide priming, *Nucleic Acids Res.* 17 (7): 2437-48 (1989).
- Gilliland, G., Analysis of cytokine mRNA and DNA: Detection and quantitation by competitive polymerase chain reaction, *PNAS*, 87(7):2725-9 (1990).
- Giusti et al., Synthesis and characterization of 5' fluorescent dye labeled oligonucleotides, *Genome Res* 2:223-227 (1993).
- Gold et al., Diversity of Oligonucleotide Functions *Annu Rev Biochem*, 64: 763-97 (1995).

(56)

References Cited

OTHER PUBLICATIONS

- Goodall, J. L. et al., Operation of Mixed-Culture Immobilized Cell Reactors for the Metabolism of Meta- and Para-Nitrobenzoate by *Comamonas* Sp. JS46 and *Comamonas* Sp. JS47, *Biotechnology and Bioengineering*, 59 (1): 21-27 (1998).
- Gordon and Balasubramanian, Solid phase synthesis—designer linkers for combinatorial chemistry: a review, *J. Chem. Technol. Biotechnol.*, 74(9):835-851 (1999).
- Grasland-Mongrain et al., Droplet coalescence in microfluidic devices, 30 pages (Jul. 2003) From internet: <http://www.eleves.ens.fr/home/grasland/rapports/stage4.pdf>.
- Green, R. and Szostak, J.W., Selection of a Ribozyme That Functions as a Superior Template in a Self Copying Reaction, *Science*, 258: 1910-5 (1992).
- Gregoriadis, G., Enzyme entrapment in liposomes, *Methods Enzymol* 44:218-227 (1976).
- Griffiths et al., Directed evolution of an extremely fast phosphotriesterase by in vitro compartmentalization, *EMBO J*, 22:24-35 (2003).
- Griffiths et al., Isolation of high affinity human antibodies directly from large synthetic repertoires, *Embo J* 13 (14):3245-60 (1994).
- Griffiths et al., Man-made enzymes—from design to in vitro compartmentalisation, *Curr Opin Biotechnol* 11:338-353 (2000).
- Griffiths, A., and Tawfik, D., Miniaturising the laboratory in emulsion droplets, *Trend Biotech* 24(9):395-402 (2006).
- Griffiths, A.D. et al., Strategies for selection of antibodies by phage display, *Curr Opin Biotechnol*, 9:102-8 (1998).
- Guatelli, J.C. et al., Isothermal, in vitro amplification of nucleic acids by a multienzyme reaction modeled after retroviral replication, *PNAS*, 87(5):1874-8 (1990).
- Guixe et al., Ligand-Induced Conformational Transitions in *Escherichia Coli* Phosphofructokinase 2: Evidence for an Allosteric Site for MgATP_{2n}, *Biochem.*, 37: 13269-12375 (1998).
- Gupta, K.C. et al., A general method for the synthesis of 3'-sulfhydryl and phosphate group containing oligonucleotides, *Nucl Acids Res* 19 (11): 3019-3026 (1991).
- Haber et al., Activity and spectroscopic properties of bovine liver catalase in sodium bis(2-ethylhexyl) sulfosuccinate/isooctane reverse micelles, *Eur J Biochem* 217(2): 567-73 (1993).
- Habig and Jakoby, Assays for differentiation of glutathione S-transferases, *Methods in Enzymology*, 77: 398-405 (1981).
- Hadd et al., Microchip Device for Performing Enzyme Assays, *Anal. Chem* 69(17): 3407-3412 (1997).
- Haddad et al., A methodology for solving physiologically based pharmacokinetic models without the use of simulation software, *Toxicol Lett.* 85(2): 113-26 (1996).
- Hagar and Spitzer, The effect of endotoxemia on concanavalin a induced alterations in cytoplasmic free calcium in rat spleen cells as determined with Fluo-3, *Cell Calcium* 13:123-130 (1992).
- Hai et al., Investigation on the release of fluorescent markers from the w/o/w emulsions by fluorescence-activated cell sorter, *J Control Release*, 96(3): 393-402 (2004).
- Haies et al., Morphometric study of rat lung cells. I. Numerical and dimensional characteristics of parenchymal cell population, *Am. Rev. Respir. Dis.* 123:533-54 (1981).
- Hall, Experimental evolution of Ebg enzyme provides clues about the evolution of catalysis and to evolutionary potential, *FEMS Microbiol Lett*, 174(1):1-8 (1999).
- Hall, The EBG system of *E. coli*: origin and evolution of a novel beta-galactosidase for the metabolism of lactose, *Genetica* 118(2-3):143-56 (2003).
- Han et al., Quantum-dot-tagged Microbeads for Multiplexed Optical Coding of Biomolecules, *Nat Biotech* 19(7): 631-635(2001).
- Handen, J.S., High-throughput screening—challenges for the future, *Drug Discov World*, 47-50 (2002).
- Handique, K. et al., On-Chip Thermopneumatic Pressure for Discrete Drop Pumping, *Analytical Chemistry*, 73:1831-1838 (2001).
- Hanes et al., Degradation of porous poly(anhydride-co-imide) microspheres and implication for controlled macromolecule delivery, *Biomaterials*, 19(1-3): 163-172(1998).
- Hanes et al., In vitro selection and evolution of functional proteins by using ribosome display, *PNAS* 94:4937-42 (1997).
- Hansen et al., A robust and scalable microfluidic metering method that allows protein crystal growth by free interface diffusion, *PNAS* 99(26):16531-16536 (2002).
- Harada et al., Monoclonal antibody G6K12 specific for membrane-associated differentiation marker of human stratified squamous epithelia and squamous cell carcinoma, *J. Oral Pathol. Med* 22(4):145-152 (1993).
- Harder, K.W. et al., Characterization and kinetic analysis of the intracellular domain of human protein tyrosine phosphatase beta (HPTP beta) using synthetic phosphopeptides, *Biochem J* 298 (Pt 2): 395-401 (1994).
- Harries et al., A Numerical Model for Segmented Flow in a Microreactor, *Int J of Heat and Mass Transfer*, 46:3313-3322 (2006).
- Harris et al., Single-molecule DNA sequencing of a viral genome, *Science* 320(5872):106-109 (2008).
- Harrison et al., Micromachining a miniaturized capillary electrophoresis-based chemical analysis system on a chip, *Science* 261(5123):895-897 (1993).
- Hasina et al., Plasminogen activator inhibitor-2: a molecular biomarker for head and neck cancer progression, *Cancer Research* 63:555-559 (2003).
- Haynes Principles of Digital PCR and Measurement Issue Oct. 15, 2012.
- Hayward et al., Dewetting Instability during the Formation of Polymersomes from Block-Copolymer-Stabilized Double Emulsions, *Langmuir*, 22(10): 4457-4461 (2006).
- He et al., Selective encapsulation of single cells and subcellular organelles into picoliter- and femtoliter-volume droplets, *Anal Chem* 77(6):1539-1544 (2005).
- Heim et al., Engineering Green Fluorescent Protein for Improved Brightness, Longer Wavelengths and Fluorescence Response Energy Transfer, *Carr. Biol*, 6(2): 178-182 (1996).
- Hellman et al., Differential tissue-specific protein markers of vaginal carcinoma, *Br J Cancer*, 100(8): 1303-131 (2009).
- Hergenrother et al., Small-Molecule Microarrays: Covalent Attachment and Screening of Alcohol-Containing Small Molecules on Glass Slides, *J. Am. Chem. Soc.*, 122: 7849-7850 (2000).
- Heyries, Kevin A, et al., Megapixel digital PCR, *Nat. Methods* 8, 649-651 (2011).
- Abstract of Sanchez et al., Breakup of Charged Capillary Jets, *Bulletin of the American Physical Society Division of Fluid Dynamics* 41:1768-1768 (1996).
- Adang, A.E. et al., The contribution of combinatorial chemistry to lead generation: an interim analysis, *Curr Med Chem* 8: 985-998 (2001).
- Advisory Action dated Sep. 9, 2014 for U.S. Appl. No. 13/679,190.
- Advisory Action for U.S. Appl. No. 11/360,845, mailed Jun. 14, 2010.
- Advisory Action for U.S. Appl. No. 11/698,298 mailed May 20, 2011.
- Affholter and F. Arnold, Engineering a Revolution, *Chemistry in Britain*, Apr. 1999, p. 48.
- Agrawal and Tang, Site-specific functionalization of oligodeoxynucleotides for non-radioactive labelling, *Tetrahedron Letters* 31:1543-1546 (1990).
- Aharoni et al., High-Throughput screens and selections of enzyme-encoding genes, *Curr Opin Chem Biol*, 9(2): 210-6 (2005).
- Ahn et al., Dielectrophoretic manipulation of drops for high-speed microfluidic sorting devices, *Applied Phys Lett* 88, 024104 (2006).
- Allen et al., High throughput fluorescence polarization: a homogeneous alternative to radioligand binding for cell surface receptors *J Biomol Screen.* 5(2):63-9 (2000).
- Altman et al., Solid-state laser using a rhodamine-doped silica gel compound, *IEEE Photonics technology letters* 3 (3):189-190 (1991).
- Amplicon Sequencing, Application Note No. 5., Feb. 2007.
- Amstutz, P. et al., In vitro display technologies: novel developments and applications. *Curr Opin Biotechnol*, 12, 400-405 (2001).

(56)

References Cited

OTHER PUBLICATIONS

- Anarbaev et al., Klenow fragment and DNA polymerase alpha-primase from calf thymus in water-in-oil microemulsions, *Biochim Biophys Acta* 1384:315-324 (1998).
- Anderson et al., Preparation of a cell-free protein-synthesizing system from wheat germ, *Methods Enzymol* 101:635-44 (1983).
- Anderson, J.E., Restriction endonucleases and modification methylases, *Curr. Op. Struct. Biol.*, 3:24-30 (1993).
- Ando, S. et al., PLGA microspheres containing plasmid DNA: preservation of supercoiled DNA via cryopreparation and carbohydrate stabilization, *J Pharm Sci*, 88(1):126-130 (1999).
- Angell et al., Silicon micromechanical devices, *Scientific American* 248:44-55 (1983).
- Anhuf et al., Determination of SMN1 and SMN2 copy number using TaqMan technology, *Hum Mutat* 22(1):74-78 (2003).
- Anna et al., Formation of dispersions using flow focusing in microchannels, *Applied Physics Letters*, 82(3): 364-366 (2003).
- Arkin, M.R. et al., Probing the importance of second sphere residues in an esterolytic antibody by phage display, *J Mol Biol* 284(4):1083-94 (1998).
- Armstrong et al., Multiple-Component Condensation Strategies for Combinatorial Library Synthesis, *Acc. Chem. Res.* 29(3):123-131 (1996).
- Ashkin and Dziedzic, Optical trapping and manipulation of viruses and bacteria, *Science* 235(4795):1517-20 (1987).
- Ashkin et al., Optical trapping and manipulation of single cells using infrared laser beams, *Nature* 330:769-771 (1987).
- Atwell, S. & Wells, J.A., Selection for Improved Subtiligases by Phage Display, *PNAS* 96: 9497-9502(1999).
- Baccarani et al., *Escherichia coli* dihydrofolate reductase: isolation and characterization of two isozymes, *Biochemistry* 16(16):3566-72 (1977).
- Baez et al., Glutathione transferases catalyze the detoxication of oxidized metabolites (o-quinones) of catecholamines and may serve as an antioxidant system preventing degenerative cellular processes, *Biochem. J* 324:25-28 (1997).
- Bagwe et al, Improved drug delivery using microemulsions: rationale, recent progress, and new horizons, *Crit Rev Ther Drug Carr Sys* 18(1):77-140 (2001).
- Baker, M., Clever PCR: more genotyping, smaller volumes, *Nature Methods* 7:351-356 (2010).
- Ball and Schwartz, CMATRIX: software for physiologically based pharmacokinetic modeling using a symbolic matrix representation system, *Comput Biol Med* 24(4):269-76 (1994).
- Ballantyne and Nixon, Selective Area Metallization by Electron-Beam Controlled Direct Metallic Deposition, *J. Vac. Sci. Technol.* 10:1094 (1973).
- Barany F., The ligase chain reaction in a PCR World, *PCR Methods and Applications* 1(1):5-16 (1991).
- Barany, F. Genetic disease detection and DNA amplification using cloned thermostable ligase, *PNAS* 88(1): 189-93 (1991).
- Baret et al., Fluorescence-activated droplet sorting (FADS): efficient microfluidic cell sorting based on enzymatic activity, *Lab on a Chip* 9:1850-1858 (2009).
- Baret et al., Kinetic aspects of emulsion stabilization by surfactants: a microfluidic analysis, *Langmuir* 25:6088-6093 (2009).
- Bass et al., Hormone Phage: An Enrichment Method for Variant Proteins With Altered Binding Properties, *Proteins* 8:309-314(1990).
- Bauer, J., Advances in cell separation: recent developments in counterflow centrifugal elutriation and continuous flow cell separation, *J Chromatography*, 722:55-69 (1999).
- Beebe et al., Functional hydrogel structures for autonomous flow control inside microfluidic channels, *Nature* 404:588-590 (2000).
- Beer et al., On-Chip, Real-Time, Single-Copy Polymerase Chain Reaction in Picoliter Droplets, *Anal. Chem.*, 79:847-8475 (2007).
- Bein, Thomas, Efficient Assays for Combinatorial methods for the Discovery of Catalysts, *Agnew. Chem. Int. Ed.* 38:3, 323-26 (1999).
- Benhar, I, et al., Highly efficient selection of phage antibodies mediated by display of antigen as Lpp-OmpA' fusions on live bacteria, *Journal of Molecular Biology*, 301 893-904 (2000).
- Benichou et al., Double Emulsions Stabilized by New Molecular Recognition Hybrids of Natural Polymers, *Polym. Adv. Tehcnol* 13:1019-1031 (2002).
- Benner, S.A., Expanding the genetic lexicon: incorporating non-standard amino acids into proteins by ribosome-based synthesis, *Trends Biotechnol* 12:158-63 (1994).
- Benning, M.M. et al., The binding of substrate analogs to phosphotriesterase. *J Biol Chem*, 275:30556-30560 (2000).
- Berman et al., An agarose gel electrophoresis assay for the detection of DNA-binding activities in yeast cell extracts, *Methods Enzymol* 155:528-37 (1987).
- Bernath et al., Directed evolution of protein inhibitors of DNA-nucleases by in vitro compartmentalization (IVC) and nano-droplet delivery, *J. Mol. Biol* 345(5):1015-26 (2005).
- Betlach, L. et al., A restriction endonuclease analysis of the bacterial plasmid controlling the EcoRI restriction and modification of DNA. *Federation Proceedings*, 35:2037-2043 (1976).
- Bibette et al., Emulsions: basic principles, *Rep. Prog. Phys.* 62:969-1033 (1999).
- Bico, Jose et al., Rise of Liquids and Bubbles in Angular Capillary Tubes, *Journal of Colloid and Interface Science*, 247:162-166 (2002).
- Bico, Jose et al., Self-Propelling Slugs, *J. Fluid Mech.*, 467:101-127 (2002).
- Park et al., Model of Formation of Monodispersed Colloids, *J. Phys. Chem. B* 105:11630-11635 (2001).
- Parker et al., Development of high throughput screening assays using fluorescence polarization: nuclear receptor-ligand-binding ligand-binding and kinase/phosphatase assays, *J Biomol Screen*, 5(2): 77-88 (2000).
- Parmley et al., Antibody-selectable filamentous fd phage vectors: affinity purification of target genes. *Gene* 73 (2):305-18 (1988).
- Pedersen et al., A method for directed evolution and functional cloning of enzymes, *PNAS* 95(18):10523-8 (1998).
- Pelham and Jackson, An efficient mRNA-dependent translation system from reticulocyte lysates, *Eur J Biochem* 67:247-56 (1976).
- Pelletier et al., An in vivo library-versus-library selection of optimized protein-protein interactions, *Nature Biotechnology*, 17:683-90 (1999).
- Peng et al., Controlled Production of Emulsions Using a Crossflow Membrane, *Particle & Particle Systems Characterization* 15:21-25 (1998).
- Perelson et al., Theoretical studies of clonal selection: minimal antibody repertoire size and reliability of self-non-self discrimination. *J Theor Biol* 81(4):645-70 (1979).
- Perez-Gilabert et al., Application of active-phase plot to the kinetic analysis of lipoxxygenase in reverse micelles, *Biochemistry J.* 288:1011-1015 (1992).
- Perrin, J., Polarisation de la lumiere de fluorescence vie moyenne des molecules dans letat excite, *J. Phys. Rad.* 1:390-401 (1926).
- Petrounia, I.P. et al., Designed evolution of enzymatic properties, *Curr Opin Biotechnol*, 11:325-330 (2000).
- Piemi et al., Transdermal delivery of glucose through hairless rat skin in vitro: effect of multiple and simple emulsions, *Int J Pharm*, 171:207-215 (1998).
- Pirrung et al., A General Method for the Spatially Defined Immobilization of Biomolecules on Glass Surfaces Using 'Caged' Biotin, *Bioconjug Chem* 7: 317-321 (1996).
- Plant (Wikipedia.com accessed Mar. 8, 2013).
- Ploem, in *Fluorescent and Luminescent Probes for Biological Activity* Mason, T. G. Ed., Academic Press, Landon, pp. 1-11, 1993.
- Pluckthun, A. et al., In vitro selection and evolution of proteins, *Adv Protein Chem*, 55: 367-403 (2000).
- Pollack et al., Electrowetting-based actuation of droplets for integrated microfluidics, *Lab Chip* 2:96-101 (2002).
- Pollack et al., Selective chemical catalysis by an antibody, *Science* 234(4783):1570-3 (1986).
- Pons et al, Synthesis of Near-Infrared-Emitting, Water-Soluble CdTeSe/CdZnS Core/Shell Quantum Dots, *Chemistry of Materials* 21(8):1418-1424 (2009).

(56)

References Cited

OTHER PUBLICATIONS

- Posner et al., Engineering specificity for folate into dihydrofolate reductase from *Escherichia coli*, *Biochemistry*, 35: 1653-63 (1996).
- Poulin and Theil, "A priori" prediction of tissue: plasma partition coefficients of drugs to facilitate the use of physiologically-based pharmacokinetic models in drug discovery, *J Pharm Sci* 89(1):16-35 (2000).
- Priest, et al. Generation of Monodisperse Gel Emulsions in a Microfluidic Device, *Applied Physics Letters*, 88:024106 (2006).
- Qi et al., Acid Beta-Glucosidase: Intrinsic Fluorescence and Conformational Changes Induced by Phospholipids and Saposin C, *Biochem.*, 37(33): 11544-11554 (1998).
- Raghuraman et al., Emulston Liquid Membranes for Wastewater Treatment: Equilibrium Models for Some Typical Metal-Extractant Systems, *Environ. Sci. Technol* 28:1090-1098 (1994).
- Ralhan, Discovery and Verification of Head-and-neck Cancer Biomarkers by Differential Protein Expression Analysis Using iTRAQ Labeling, Multidimensional Liquid Chromatography, and Tandem Mass Spectrometry, *Mol Cell Proteomics* 7(6):1162-1173 (2008).
- Ramsey, J.M., The burgeoning power of the shrinking laboratory, *Nat Biotechnol* 17(11):1061-2 (1999).
- Ramstrom and Lehn, Drug discovery by dynamic combinatorial libraries, *Nat Rev Drug Discov* 1:26-36 (2002).
- Raushel, F.M. et al., Phosphotriesterase: an enzyme in search of its natural substrate, *Adv Enzymol Relat Areas Mol Biol*, 74: 51-93 (2000).
- Rech et al., Introduction of a yeast artificial chromosome vector into *Sarrachomyces cerevisia* by electroporation, *Nucleic Acids Res* 18:1313 (1990).
- Reyes et al., Micro Total Analysis Systems. 1. Introduction, Theory and Technology, *Anal Chem* 74(12):2623-2636 (2002).
- Riess, J.S., Fluorous micro- and nanophases with a biomedical perspective, *Tetrahedron* 58(20):4113-4131 (2002).
- Roach et al., Controlling nonspecific protein adsorption in a plug-based microfluidic system by controlling interfacial chemistry using fluorous-phase surfactants, *Anal. Chem.* 77:785-796 (2005).
- Roberts & Ja, In vitro selection of nucleic acids and proteins: What are we learning, *Curr Opin Struct Biol* 9(4): 521-9 (1999).
- Roberts et al., Simian virus 40 DNA directs synthesis of authentic viral polypeptides in a linked transcription-translation cell-free system 72(5):1922-1926 (1975).
- Roberts, et al., RNA-peptide fusion for the in vitro selection of peptides and proteins, *PNAS* 94:12297-302 (1997).
- Roberts, J.W., Termination factor for RNA synthesis, *Nature*, 224: 1168-74 (1969).
- Roberts, R.W. Totally in vitro protein selection using mRNA-protein fusions and ribosome display. *Curr Opin Chem Biol* 3(3), 268-73 (1999).
- Rodriguez-Antona et al., Quantitative RT-PCR measurement of human cytochrome P-450s: application to drug induction studies. *Arch. Biochem. Biophys.*, 376:109-116 (2000).
- Rolland et al., Fluorescence Polarization Assay by Flow Cytometry, *J. Immunol. Meth.*, 76(1): 1-10 (1985).
- Rosenberg et al., Inhibition of Human Factor IX by Human Antithrombin, *J Biol Chem*, 250: 4755-64 (1975).
- Rosenberg et al., Termination of transcription in bacteriophage lambda, *J Biol Chem*, 250: 4755-64 (1975).
- Rosenberry, T.L., Acetylcholinesterase, *Adv Enzymol Relat Areas Mol Biol*, 43: 103-218 (1975).
- Rotman, Measurement of activities of single molecules of beta-galactosidase, *PNAS*, 47:1981-91 (1961).
- Russon et al., Single-nucleotide polymorphism analysis by allele-specific extension of fluorescently labeled nucleotides in a microfluidic flow-through device, *Electrophoresis*, 24:158-61 (2003).
- Sadtler et al., Achieving stable, reverse water-in-fluorocarbon emulsions. *Angew Chem Int Ed* 35:1976-1978 (1996).
- Saiki, R.K., et al, Primer directed enzymatic amplification of DNA with a thermostable DNA polymerase. *Science* 239 (4839):487-91 (1988).
- Sakamoto, Rapid and simple quantification of bacterial cells by using a microfluidic device, *Appl Env Microb.* 71:2 (2005).
- Sanchez et al., Breakup of Charged Capillary Jets, *Bulletin of the American Physical Society Division of Fluid Dynamics* 41:1768-1768 (1996).
- Sano, T. et al., Immuno-PCR—Very sensitive antigen-detection by means of specific antibody—DNA conjugates. *Science* 258(5079), 120-122 (1992).
- SantaLucia, A unified view of polymer, dumbbell, and oligonucleotide DNA nearest-neighbor thermodynamics, *PNAS* 95(4):1460-5 (1998).
- Santra et al., Fluorescence lifetime measurements to determine the core-shell nanostructure of FITC-doped silica nanoparticles: an optical approach to evaluate nanoparticle photostability, *J Luminescence* 117(1):75-82 (2006).
- Schatz et al., Screening of peptide libraries linked to lac repressor, *Methods Enzymol* 267: 171-91 (1996).
- Schneegass et al., Miniaturized flow-through PCR with different template types in a silicone chip thermocycler, *Lab on a Chip, Royal Soc of Chem*, 1:42-9 (2001).
- Schubert et al., Designer Capsules, *Nat Med* 8:1362 (2002).
- Schweitzer et al., Immunoassays with rolling circle DNA amplification: A versatile platform for ultrasensitive antigen detection, *PNAS* 97(18), 10113-10119 (2000).
- Schweitzer, B. et al., Combining nucleic acid amplification and detection. *Curr Opin Biotechnol* 12(1):21-7 (2001).
- Scott, R.L., The Solubility of Fluorocarbons, *J. Am. Chem. Soc.*, 70: 4090-4093 (1948).
- Seethala and Menzel, Homogeneous, Fluorescence Polarization Assay for Src-Family Tyrosine Kinases, *Anal Biochem* 253(2):210-218 (1997).
- Seiler et al., Planar glass chips for capillary electrophoresis: repetitive sample injection, quantitation, and separation efficiency, *Anal Chem* 65(10):1481-1488 (1993).
- Selwyn M. J., A simple test for inactivation of an enzyme during assay, *Biochim Biophys Acta* 105:193-195 (1965).
- Seo et al., Microfluidic consecutive flow-focusing droplet generators, *Soft Matter*, 3:986-992 (2007).
- Seong and Crooks, Efficient Mixing and Reactions Within Microfluidic Channels Using Microbead-Supported Catalysts, *J Am Chem Soc* 124(45):13360-1 (2002).
- Seong et al., Fabrication of Microchambers Defined by Photopolymerized Hydrogels and Weirs Within Microfluidic Systems: Application to DNA Hybridization, *Analytical Chem* 74(14):3372-3377 (2002).
- Sepp et al., Microbead display by in vitro compartmentalisation: selection for binding using flow cytometry, *FEBS Letters* 532:455-58 (2002).
- Serpensu et al., Reversible and irreversible modification of erythrocyte membrane permeability by electric field, *Biochim Biophys Acta* 812(3):779-785 (1985).
- Shapiro, H.M., Multistation multiparameter flow cytometry: a critical review and rationale, *Cytometry* 3: 227-243 (1983).
- Shestopalov et al., Multi-Step Synthesis of Nanoparticles Performed on Millisecond Time Scale in a Microfluidic Droplet-Based System, *The Royal Society of Chemistry* 4:316-321(2004).
- Shim, Jung-uk, et al., Using Microfluidics to Decoupled Nucleation and Growth of Protein Crystals, *Cryst. Growth, Des.* 2007; 7(11): 2192-2194.
- Shtern V, and Hussain F., Hysteresis in swirling jets, *J. Fluid Mech.* 309:1-44 (1996).
- Sia & Whitesides, Microfluidic devices fabricated in poly(dimethylsiloxane) for biological studies, *Electrophoresis* 24 (21):3563-3576 (2003).
- Sidhu, S.S., Phage display in pharmaceutical biotechnology, *Curr Opin Biotech* 11:610-616 (2000).
- Siemering et al., Mutations that suppress the thermosensitivity of green fluorescent protein, *Current Biology* 6:1653-1663 (1996).

(56)

References Cited

OTHER PUBLICATIONS

- Silva-Cunha et al., W/O/W multiple emulsions of insulin containing a protease inhibitor and an absorption enhancer: biological activity after oral administration to normal and diabetic rats, *Int J Pharm* 169:33-44 (1998).
- Sims et al., Immunopolymerase chain reaction using real-time polymerase chain reaction for detection, *Anal. Biochem.* 281(2):230-2 (2000).
- Slappendel et al., Normal cations and abnormal membrane lipids in the red blood cells of dogs with familial stomatocytosis hypertrophic gastritis, *Blood* 84:904-909 (1994).
- Slob et al., Structural identifiability of PBPK models: practical consequences for modeling strategies and study designs, *Crit Rev Toxicol.* 27(3):261-72 (1997).
- Smith et al., Direct mechanical measurements of the elasticity of single DNA molecules by using magnetic beads, *Science* 258(5085):1122-1126 (1992).
- Smith et al., Fluorescence detection in automated DNA sequence analysis, *Nature* 321:674-679 (1986).
- Smith et al., Phage display, *Chemical Reviews* 97(2), 391-410 (1997).
- Smith et al., The synthesis of oligonucleotides containing an aliphatic amino group at the 5' terminus: synthesis of fluorescent DNA primers for use in DNA sequence analysis, *Nucl. Acid Res.* 13:2399-2412 (1985).
- Smith G.P., Filamentous fusion phage: novel expression vectors that display cloned antigens on the virion surface, *Science* 228(4705):1315-7(1985).
- Smyth et al., Markers of apoptosis: methods for elucidating the mechanism of apoptotic cell death from the nervous system, *Biotechniques* 32:648-665 (2000).
- Sohn, et al, Capacitance cytometry: Measuring biological cells one by one, *PNAS* 97(20):10687-10690 (2000).
- Somasundaram and Ramalingam, Gain studies of Rhodamine 6G dye doped polymer laser, *J Photochem Photobiol* 125(1-3):93-98 (1999).
- Song et al., A microfluidic system for controlling reaction networks in time, *Angew. Chem. Int. Ed.* 42(7):768-772 (2003).
- Song et al., Experimental Test of Scaling of Mixing by Chaotic Advection in Droplets Moving Through Microfluidic Channels, *App Phy Lett* 83(22):4664-4666 (2003).
- Song, H. and Ismagilov, R.F., Millisecond kinetics on a microfluidic chip using nanoliters of reagents, *J Am Chem Soc.* 125: 14613-14619 (2003).
- Soni and Meller, Progress toward ultrafast DNA sequencing using solid-state nanopores, *Clin Chem* 53:1996-2001 (2007).
- Soumillion et al., Novel concepts for the selection of catalytic activity. *Curr Opin Biotechnol* 12:387-394 (2001).
- Soumillion et al., Selection of B-lactomase on filamentous bacteriophage by catalytic activity, *J Mol Biol.* 237:415-22 (1994).
- Sproat et al., The synthesis of protected 5'-mercapto-2',5'-dideoxyribonucleoside-3'-0-phosphorainidites, uses of 5'-mercapto-oligodeoxyribonucleotides, *Nucleic Acids Res* 15:4837-4848 (1987).
- Stauber, et a., Rapid generation of monoclonal antibody-secreting hybridomas against African horse sickness virus by in vitro immunization ion and the fusion/cloning technique, *J. Immunol. Meth* 161(2):157-168 (1993).
- Stemmer, W.P., DNA shuffling by random fragmentation and reassembly: in vitro recombination for molecular evolution. *PNAS* 91(22):10747-51(1994).
- Stemmer, W.P., Rapid evolution of a protein in vitro by DNA shuffling, *Nature* 370(6488):389-91 (1994).
- Stober et al., Controlled growth of monodisperse silica spheres in the micron size range, *J Colloid and Interface Sci* 26 (1):62-69 (1968).
- Stofko, H.R. et al., A single step purification for recombinant proteins. Characterization of microtubule associated protein (MAP2) fragment which associates with the type II cAMP-dependent protein kinase, *Febs Lett* 302: 274-278 (1992).
- Stone et al., Engineering flows in small devices: Microfluidics toward a lab-on-a-chip, *Ann. Rev. Fluid Mech.* 36:381-441 (2004).
- Strizhkov et al., PCR amplification on a microarray of gel-immobilized oligonucleotides: Detection of bacterial toxin- and drug-resistant genes and their mutations, *BioTechniques* 29(4):844-857 (2000).
- Stroock et al., Chaotic mixer for microchannels, *Science* 295(5555):647-651 (2002).
- Studer et al., Fluorous Synthesis: A Fluorous-Phase Strategy for Improving Separation Efficiency in Organic Synthesis, *Science* 275: 823-826 (1997).
- Mueth et al., Origin of stratification in creaming emulsions, *Physical Review Letters* 77(3):578-581 (1996).
- Mulbry, W.W. et al., Parathion hydrolase specified by the *Flavobacterium opd* gene: relationship between the gene and protein. *J Bacteriol.* 171: 6740-6746 (1989).
- Mulder et al., Characterization of two human monoclonal antibodies reactive with HLA-B12 and HLA-B60, respectively, raised by in vitro secondary immunization of peripheral blood lymphocytes, *Hum. Immunol* 36(3):186-192 (1993).
- Murinae (Wikipedia.com accessed Mar. 18, 2013).
- Nakano et al., High speed polymerase chain reaction in constant flow, *Biosci Biotech and Biochem.* 58:349-52 (1994).
- Nakano et al., Single-molecule PCR using water-in-oil emulsion, *J Biotech.* 102:117-24 (2003).
- Nakano et al., Single-molecule reverse transcription polymerase chain reaction using water-in-oil emulsion, *J Biosci Bioeng* 99:293-295 (2005).
- Nametkin, S.N. et al., Cell-free translation in reversed micelles, *FEB Letters.* 309(3):330-32 (1992).
- Narang et al, Improved phosphotriester method for the synthesis of gene fragments, *Methods Enzymol.* 68:90-98 (1979).
- Nelson, P. S., et al., Bifunctional oligonucleotide probes synthesized using a novel CPG support are able to detect single base pair mutations, *Nucl Acids Res* 17(18): 7187-7194 (1989).
- Nemoto et al., In vitro virus: bonding of mRNA bearing puromycin at the 3 terminal end to the C-terminal end of its encoded protein on the ribosome in vitro, *Federation of European Biochemical Societies.* 414:405-8 (1997).
- Ness, J.E. et al., Molecular Breeding: the natural approach to protein design. *Adv Protein Chem.* 55: 261-292 (2000).
- Ng et al., Protein crystallization by capillary counter—diffusion for applied crystallographic structure determination, *J. Stud. Biol.* 142:218-231(2003).
- Ng, B.L. et al., Factors affecting flow karyotype resolution, *Cytometry, Part A* 69A: 1028-1036 (2006).
- Nguyen et al., Optical detection for droplet size control in microfluidic droplet-based analysis systems, *Sensors and Actuators B* 117(2):431-436 (2006).
- Nihant et al., Polylactide Microparticles Prepared by Double Emulsion/Evaporation Technique. I. Effect of Primary Emulsion Stability, *Pharmaceutical Research.* 11(10):1479-1484 (1994).
- Nisisako et al., Controlled formulation of monodisperse double emulsions in a multiple-phase microfluidic system, *Sot Matter.* 1:23-27 (2005).
- Nisisako et al., Microstructured Devices for Preparing Controlled Multiple Emulsions. *Chem. Eng. Technol* 31 (8):1091-1098 (2008).
- Nisisako, Takasi et al., Droplet Formation in a MicroChannel NetWork, *Lab on a Chip.* vol. 2, 2002, pp. 24-26.
- Nissim, A. et al., Antibody fragments from a single pot phage display library as immunochemical reagents, *Embo J.* 13:692-8 (1994).
- Nof and Shea, Drug-releasing scaffolds fabricated from drug-loaded microspheres, *J. Biomed Mater Res* 59:349-356 (2002).
- Norman, A., Flow Cytometry, *Med. Phys.*, 7(6):609-615 (1980).
- Notice of Refusal for Application No. 04782399.2 dated Apr. 10, 2013 (10 pages).
- Oberholzer et al., Enzymatic RNA replication in self-reproducing vesicles: an approach to a minimal cell, *Biochem Biophys Res Commun* 207(1):250-7 (1995).
- Oberholzer et al., Polymerase chain reaction in liposomes, *Chem. Biol.* 2(10):677-82 (1995).

(56)

References Cited

OTHER PUBLICATIONS

- Obukowicz, M.G. et al., Secretion and export of IGF-1 in *Escherichia coli* strain JM101, *Mol Gen Genet*, 215:19-25 (1988).
- Office Action for 11/360,845 Dated Nov. 19, 2013, 16 pages.
- Office Action for 13/679,190 dated Dec. 2, 2013, 13 pages.
- Office Action for U.S. Appl. No. 11/246,911 mailed Feb. 8, 2011.
- Office Action for U.S. Appl. No. 11/360,845 mailed Apr. 26, 2011.
- Office Action for U.S. Appl. No. 11/360,845 mailed Aug. 4, 2010.
- Office Action for U.S. Appl. No. 11/698,298, mailed Jun. 29, 2011.
- Office Action mailed Jun. 5, 2014 for U.S. Appl. No. 13/679,190.
- Ogura, Y., Catalase activity at high concentrations of hydrogen peroxide, *Archs Biochem Biophys*, 57: 288-300 (1955).
- Oh et al., Distribution of Macropores in Silica Particles Prepared by Using Multiple Emulsions, *Journal of Colloid and Interface Science*, 254(1): 79-86 (2002).
- Oh et al., World-to-chip microfluidic interface with built-in valves for multichamber chip-based PCR assays, *Lab Chip*, 2005, 5, 845-850.
- Okushima et al. Controlled production of monodisperse double emulsions by two -step droplet breakup in microfluidic devices, *Langmuir* 20(23): 9905-8 (2004).
- Olsen et al., Function-based isolation of novel enzymes from a large library, *Nat Biotechnol* 13(10):1071-4 (2000).
- Olsen et al., Function-based isolation of novel enzymes from a large library, *Nat Biotechnol* 13(10):1071-4 (2000).
- Omburo, G.A. et al., Characterization of the zinc binding site of bacterial phosphotriesterase, *J of Biological Chem*, 267:13278-83 (1992).
- Original and translated Notice of Final Rejection dated Nov. 19, 2013 for Japanese Patent Application 2008-550290 (5 pages).
- Original and translated Notice of Reasons for Rejection dated Apr. 10, 2013 for Japanese Patent Application 2008-550290 (6 pages).
- Oroskar et al., Detection of immobilized amplicons by ELISA-like techniques, *Clin. Chem.* 42:1547-1555 (1996).
- Ostermeier, M. et al., A combinatorial approach to hybrid enzymes independent of DNA homology, *Nat Biotechnol*, 17 (12):1205-9 (1999).
- Ouelette, A new wave of microfluidic devices, *Indust Physicist* pp. 14-17 (2003).
- Pabit et al., Laminar-Flow Fluid Mixer for Fast Fluorescence Kinetics Studies, *Biophys J* 83:2872-2878 (2002).
- Paddison et al., Stable suppression of gene expression by RNAi in mammalian cells, *PNAS* 99(3):1443-1448 (2002).
- Pannacci et al., Equilibrium and Nonequilibrium States in Microfluidic Double Emulsions *Physical Review Letters*, 101 (16):164502 (2008).
- Park et al., Cylindrical compact thermal-cycling device for continuous-flow polymerase chain reaction, *Anal Chem, ACS*, 75:6029-33 (2003).
- Xu, S. et al., Generation of monodisperse particles by using microfluidics: control over size, shape, and composition, *Angew. Chem. Int. Ed.* 44:724-728 (2005).
- Yamagishi, J. et al., Mutational analysis of structure-activity relationships in human tumor necrosis factor- α , *Protein Eng*, 3:713-9 (1990).
- Yamaguchi et al., Insulin-loaded biodegradable PLGA microcapsules: initial burst release controlled by hydrophilic additives, *Journal of Controlled Release*, 81(3): 235-249 (2002).
- Yelamos, J. et al., Targeting of non-Ig sequences in place of the V segment by somatic hypermutation. *Nature* 376 (6537):225-9 (1995).
- Yershov et al., DNA analysis and diagnostics on oligonucleotide microchips, *PNAS* 93(10):4913-4918 (1996).
- Yonezawa et al., DNA display for in vitro selection of diverse peptide libraries, *Nucleic Acids Research*, 31(19): e118 (2003).
- Yu et al. Responsive biomimetic hydrogel valve for microfluidics. *Appl. Phys. Lett* 78:2589-2591 (2001).
- Yu et al., Quantum dot and silica nanoparticle doped polymer optical fibers, *Optics Express* 15(16):9989-9994 (2007).
- Yu et al., Specific inhibition of PCR by non-extendable oligonucleotides using a 5' to 3' exonuclease—deficient DNA polymerase, *Biotechniques* 23(4):714-6, 718-20 (1997).
- Zaccolo, M. et al., An approach to random mutagenesis of DNA using mixtures of triphosphate derivatives of nucleoside analogues. *J Mol Biol* 255(4):589-603 (1996).
- Zakrzewski, S.F., Preparation of tritiated dihydrofolic acid of high specific activity, *Methods Enzymol*, 539 (1980).
- Zaug and Cech, The intervening sequence RNA of *Tetrahymena* is an enzyme, *Science* 231(4737):470-5 (1986).
- Zaug and Cech, The *Tetrahymena* intervening sequence ribonucleic acid enzyme is a phosphotransferase and an acid phosphatase, *Biochemistry* 25(16):4478-82 (1986).
- Zaug et al., The *Tetrahymena* ribozyme acts like an RNA restriction endonuclease, *Nature* 324(6096):429-33 (1986).
- Zhang et al., A Simple Statistical Parameter for Use in Evaluation and Validation of High Throughput Screening Assays, *Journal of Biomolecular Screening*, 4(2): 67-73 (1999).
- Zhang, Z.Y., Substrate specificity of the protein tyrosine phosphatases, *PNAS* 90: 4446-4450 (1993).
- Zhao, B. et al., Control and Applications of Immiscible Liquids in Microchannels, *J. Am. Chem. Soc*, vol. 124:5284-5285 (2002).
- Zhao, H. et al., Molecular evolution by staggered extension process (STEP) in vitro recombination. *Nat Biotechnol* 16 (3):258-61 (1998).
- Zheng et al., A Droplet-Based, Composite PDMS/Glass Capillary Microfluidic System for Evaluating Protein Crystallization Conditions by Microbatch and Vapor-Diffusion Methods with On-Chip X-Ray Diffraction, *Angew. Chem.*, 116:1-4, (2004).
- Zheng et al., A Microfluidic Approach for Screening Submicroliter Volumes against Multiple Reagents by Using Performed Arrays of Nanoliter Plugs in a Three-Phase Liquid/Liquid/Gas Flow, *Angew. Chem. Int. Ed.*, 44(17): 2520-2523 (2005).
- Zheng et al., Formation of Droplets of Alternating Composition in Microfluidic Channels and Applications to Indexing of Concentrations in Droplet-Based /Assays, *Anal. Chem.*, 76: 4977-4982 (2004).
- Zheng et al., Screening of Protein Crystallization Conditions on a Microfluidic Chip Using Nanoliter-Size Droplets, *J Am Chem Soc* 125(37):11170-11171 (2003).
- Zimmermann et al., Dielectric Breakdown of Cell Membranes, *Biophys J* 14(11):881-889 (1974).
- Zimmermann et al., Microscale Production of Hybridomas by Hypo-Osmolar Electrofusion, *Hum. Antibod. Hybridomas*, 3(1): 14-18 (1992).
- Zimmermann, Bernhard G., et al., Digital PCR: a powerful new tool for noninvasive prenatal diagnosis?, *Prenat Diagn* 28, 1087-1093 (2008).
- Zubay, G., In vitro synthesis of protein in microbial systems, *Annu Rev Genet*, 7: 267-87 (1973).
- Zubay, G., The isolation and properties of CAP, the catabolite gene activator, *Methods Enzymol*, 65: 856-77 (1980).
- Zuckermann, R. et al., Efficient Methods for Attachment of Thiol-Specific Probes to the 3-end of Synthetic Oligodeoxyribonucleotides, *Nucleic Acids Res.* 15:5305-5321 (1987).
- Blattner and Dahlberg, RNA synthesis startpoints in bacteriophage lambda: are the promoter and operator transcribed, *Nature New Biol* 237(77):227-32 (1972).
- Boder et al., Yeast surface display for screening combinatorial polypeptide libraries, *Nat Biotechnol* 15(6):553-7 (1997).
- Bougueleret, L. et al., Characterization of the gene coding for the EcoRV restriction and modification system of *Escherichia coli*, *Nucleic Acids Res*, 12(8):3659-76 (1984).
- Boyum, A., Separation of leukocytes from blood and bone marrow. Introduction, *Scand J Clin Lab Invest Suppl* 97:7 (1968).
- Branebjerg et al., Fast mixing by lamination, *MEMS Proceedings 9th Ann Workshop, San Diego, Feb. 11-15, 1996*, 9:441-446 (1996).
- Braslaysky et al., Sequence information can be obtained from single DNA molecules, *PNAS* 100(7):3960-3964 (2003).
- Bringer et al., Microfluidic Systems for Chemical Kinetics That Rely on Chaotic Mixing in Droplets, *Philos Transact a Math Phys Eng Sci* 362:1-18 (2004).
- Brody et al., A self-assembled microlensing rotational probe, *Applied Physics Letters*, 74:144-46 (1999).

(56)

References Cited

OTHER PUBLICATIONS

- Brown et al., Chemical synthesis and cloning of a tyrosine tRNA gene, *Methods Enzymol* 68:109-151 (1979).
- Bru, R. et al., Catalytic activity of elastase in reverse micelles, *Biochem Mol Bio Int*, 31(4):685-92 (1993).
- Bru, R. et al., Product inhibition of alpha-chymotrypsin in reverse micelles. *Eur J Biochem* 199(1):95-103 (1991).
- Brummelkamp et al., A system for stable expression of short interfering RNAs in mammalian cells, *Science* 296 (5567):550-3 (2002).
- Buckpitt et al., Hepatic and pulmonary microsomal metabolism of naphthalene to glutathione adducts: factors affecting the relative rates of conjugate formation, *J. Pharmacol. Exp. Ther.* 231:291-300 (1984).
- Buican et al., Automated single-cell manipulation and sorting by light trapping, *Applied Optics* 26(24):5311-5316 (1987).
- Burbaum, J., Miniaturization technologies in HTS: how fast, how small, how soon *Drug Discov Today* 3:313-322 (1998).
- Burns et al., Microfabricated structures for integrated DNA analysis, *Proc. Natl. Acad. Sci. USA*, 93:5556-5561(1996).
- Burns, J.R. et al., The Intensification of Rapid Reactions in Multiphase Systems Using Slug Flow in Capillaries, *Lab on a Chip*, 1:10-15 (2001).
- Burns, Mark et al., An Integrated Nanoliter DNA Analysis Device, *Science*, 282:484-487(1998).
- Byrnes, P.J. et al., Sensitive fluorogenic substrates for the detection of trypsin-like proteases and pancreatic elastase, *Anal Biochem*, 126:447 (1982).
- Cahill et al., Polymerase chain reaction and Q beta replicase amplification, *Clin Chem* 37(9):1482-5 (1991).
- Caldwell, S.R. et al., Limits of diffusion in the hydrolysis of substrates by the phosphodiesterase from *Pseudomonas diminuta*, *Biochemistry*, 30: 7438-7444 (1991).
- Calvert, P., Inkjet printing for materials and devices, *Chem Mater* 13: 3299-3305 (2001).
- Caruthers, Gene synthesis machines: DNA chemistry and its uses, *Science* 230:281-285 (1985).
- Chakrabarti, A.C. et al., Production of RNA by a polymerase protein encapsulated within phospholipid vesicles, *J Mol Evol*, 39(6):555-9 (1994).
- Chamberlain and Ring, Characterization of T7-specific ribonucleic acid polymerase. 1. General properties of the enzymatic reaction and the template specificity of the enzyme, *J Biol Chem* 248:2235-44 (1973).
- Chan, Emory M. et al., Size-Controlled Growth of CdSe Nanocrystals in Microfluidic Reactors, *Nano Letters*, 3 (2):199-201(2003).
- Chang and Su, Controlled double emulsification utilizing 3D PDMS microchannels, *Journal of Micromechanics and Microengineering* 18:1-8 (2008).
- Chang, T.M., Recycling of NAD(P) by multienzyme systems immobilized by microencapsulation in artificial cells, *Methods Enzymol*, 136(67):67-82 (1987).
- Chao et al., Control of Concentration and Volume Gradients in Microfluidic Droplet Arrays for Protein Crystallization Screening, 26th Annual International Conference of the IEEE Engineering in Medicine and Biology Society, San Francisco, California Sep. 1-5, 2004.
- Chao et al., Droplet Arrays in Microfluidic Channels for Combinatorial Screening Assays, Hilton Head 2004: A Solid State Sensor, Actuator and Microsystems Workshop, Hilton Head Island, South Carolina, Jun. 6-10, 2004.
- Chapman et al., In vitro selection of catalytic RNAs, *Curr. op. Struct. Biol.*, 4:618-22 (1994).
- Chayen, Crystallization with oils: a new dimension in macromolecular crystal growth *Journal of Crystal Growth*, 196:434-441(1999).
- Chen et al., Capturing a Photoexcited Molecular Structure Through Time-Domain X-ray Absorption Fine Structure, *Science* 292(5515):262-264 (2001).
- Chen et al., Microfluidic Switch for Embryo and Cell Sorting the 12th International Conference on Solid State Sensors, Actuators, and Microsystems, Boston, MA Jun. 8-12, 2003 *Transducers*, 1: 659-662 (2003).
- Chen-Goodspeed et al., Structural Determinants of the substrate and stereochemical specificity of phosphotriesterase, *Biochemistry*, 40(5):1325-31 (2001).
- Chen-Goodspeed, M. et al., Enhancement, relaxation, and reversal of the stereoselectivity for phosphotriesterase by rational evolution of active site residues, *Biochemistry*, 40: 1332-1339 (2001b).
- Cheng, Z., et al, Electro flow focusing in microfluidic devices, *Microfluidics Poster*, presented at DBAS, *Frontiers in Nanoscience*, presented Apr. 10, 2003.
- Chetverin and Spirin, Replicable RNA vectors: prospects for cell-free gene amplification, expression, and cloning, *Prog Nucleic Acid Res Mol Biol*, 51:225-70 (1995).
- Chiang, C.M. et al., Expression and purification of general transcription factors by FLAG epitope-tagging and peptide elution, *Pept Res*, 6:62-64 (1993).
- Chiba et al., Controlled protein delivery from biodegradable tyrosine-containing poly(anhydride-co-imide) microspheres, *Biomaterials*, 18(13):893-901 (1997).
- Chiou et al., A closed-cycle capillary polymerase chain reaction machine, *Analytical Chemistry*, American Chemical Society, 73:2018-21 (2001).
- Chiu et al., Chemical transformations in individual ultrasmall biomimetic containers, *Science*, 283:1892-1895 (1999).
- Chou et al., A microfabricated device for sizing and sorting DNA molecules 96:11-13(1998).
- Clackson, T. et al., In vitro selection from protein and peptide libraries, *Trends Biotechnol*, 12:173-84 (1994).
- Clausell-Tormos et al., Droplet-based microfluidic platforms for the encapsulation and screening of Mammalian cells and multicellular organisms, *Chem Biol* 15(5):427-437 (2008).
- Cohen, S. et al., Controlled delivery systems for proteins based on poly(lactic/glycolic acid) microspheres, *Pharm Res*, 8(6):713-720 (1991).
- Collins et al., Optimization of Shear Driven Droplet Generation in a Microfluidic Device, ASME International Mechanical Engineering Congress and R&D Expo, Washington (2003).
- Collins, J. et al., Microfluidic flow transducer based on the measurements of electrical admittance, *Lab on a Chip*, 4:7-10 (2004).
- Compton, J., Nucleic acid sequence-based amplification, *Nature*, 350(6313):91-2 (1991).
- Cormack, B.P. et al., FACS—optimized mutants of the green fluorescent protein (GFP), *Gene* 173(1):33-38 (1996).
- Hildebrand et al., Liquid-Liquid Solubility of Perfluoromethylcyclohexane with Benzene, Carbon Tetrachloride, Chlorobenzene, Chloroform and Toluene, *J. Am. Chem. Soc.* 71: 22-25 (1949).
- Hindson, Benjamin J., et al., High-Throughput Droplet Digital PCR System for Absolute Quantitation of DNA Copy Number, *Anal. Chem.*, 83, 8604-8610 (2011).
- Hjelmfelt et al, Pattern-Recognition in Coupled Chemical Kinetic Systems, *Science*, 260(5106):335-337 (1993).
- Ho, S.N. et al., Site-directed mutagenesis by overlap extension using the polymerase chain reaction, *Gene*, 77(1):51-9 (1989).
- Hoang, Physiologically based pharmacokinetic models: mathematical fundamentals and simulation implementations, *Toxicol Lett* 79(1-3):99-106 (1995).
- Hochuli et al., New metal chelate adsorbent selective for proteins and peptides containing neighbouring histidine residues, *J Chromatogr* 411: 177-84 (1987).
- Holmes et al., Reagents for Combinatorial Organic Synthesis: Development of a New O-Nitrobenzyl Photolabile Linder for Solid Phase Synthesis, *J. OrgChem.*, 60: 2318-2319(1995).
- Holtze, C., et al., Biocompatible surfactants for water-in-fluorocarbon emulsions, *Lab Chip*, 2008, 8, 1632-1639.
- Hong, S.B. et al., Stereochemical constraints on the substrate specificity of phosphodiesterase, *Biochemistry*, 38: 1159-1165 (1999).

(56)

References Cited

OTHER PUBLICATIONS

- Hoogenboom et al., Multi-subunit proteins on the surface of filamentous phage: methodologies for displaying antibody (Fab) heavy and light chains, *Nucl Acids Res.*, 91: 4133-4137 (1991).
- Hoogenboom, H.R., Designing and optimizing library selection strategies for generating high-affinity antibodies, *Trends Biotechnol*, 15:62-70 (1997).
- Hopfinger & Lasheras, Explosive Breakup of a Liquid Jet by a Swirling Coaxial Jet, *Physics of Fluids* 8(7):1696-1700 (1996).
- Hopman et al., Rapid synthesis of biotin-, digoxigenin-, trinitrophenyl-, and fluorochrome-labeled tyramides and their application for in situ hybridization using CARD amplification, *J of Histochem and Cytochem*, 46(6):771-77 (1998).
- Horton et al., Engineering hybrid genes without the use of restriction enzymes: gene splicing by overlap extension, *Gene* 77(1):61-8 (1989).
- Hosokawa, Kazuo et al., Handling of Picoliter Liquid Samples in a Poly(dimethylsiloxane)-Based Microfluidic Device, *Analytical Chemistry*, 71(20):4781-4785 (1999).
- How many species of bacteria are there(wisegeek.com; accessed Sep. 23, 2011).
- Hsu et al., Comparison of process parameters for microencapsulation of plasmid DNA in poly(D, L-lactic-co-glycolic acid) microspheres, *J Drug Target*, 7:313-23 (1999).
- Huang L. R. et al., Continuous particle separation through deterministic lateral displacement, *Science* 304 (5673):987-990 (2004).
- Huang, Z. et al., A sensitive competitive Elisa for 2,4-dinitrophenol using 3,6-fluorescein diphosphate as a fluorogenic substrate, *J Immunol Meth*, 149:261 (1992).
- Huang, Z.J., Kinetic assay of fluorescein mono-beta-D-galactosidase hydrolysis by beta-galactosidase: a front-face measurement for strongly absorbing fluorogenic substrates, *Biochemistry*, 30:8530-4 (1991).
- Hubert et al. Data Concordance from a Comparison between Filter Binding and Fluorescence Polarization Assay Formats for Identification of RUOck-II Inhibitors, *J biomol Screen* 8(4):399-409 (2003).
- Huebner, A. et al., Quantitative detection of protein expression in single cells using droplet microfluidics, *Chem Com* 12:1218-1220 (2007).
- Hug et al. Measurement of the number of molecules of a single mRNA species in a complex mRNA preparation. *J Theor Biol.*; 221(4):615-24 (2003).
- Hung et al., Optimization of Droplet Generation by controlling PDMS Surface Hydrophobicity, 2004 ASME International Mechanical Engineering Congress and Rd&D Expo, Nov. 13-19, Anaheim, CA (2004).
- Hung, et al, Controlled Droplet Fusion in Microfluidic Devices, *MicroTAS*, Sep. 26-30, 2004, Malmo, Sweden (2004).
- Hutchison et al., Cell-free cloning using Phi29 polymerase, *PNAS* 102(48):17332-17336 (2005).
- Ibrahim, S.F. et al., High-speed cell sorting: fundamentals and recent advances, *Curr Opin Biotchnol*, 14(1):5-12 (2003).
- Ikeda et al., Bioactivation of tegafur to 5-fluorouracil is catalyzed by cytochrome P-450 2A6 in human liver microsomes in vitro, *Clin Cancer Res* 6(11):4409-4415 (2000).
- Inai et al., Immunohistochemical detection of an enamel protein-related epitope in rat bone at an early stage of osteogenesis, *Histochemistry* 99(5):335-362 (1993).
- International Preliminary Report of Patentability for PCTUS2010061741 Mailed Sep. 16, 2011(4 pages).
- International Preliminary Report on Patentability mailed Sep. 20, 2007, for PCT/US2006/007772.
- International Preliminary Report on Patentability mailed Sep. 20, 2007, for PCT/US2006/007772 (11 pages).
- International Preliminary Report on Patentability PCT/US2004/027912 dated Jan. 26, 2005, 7 pages.
- International Search Report and Written Opinion for PCT/US11/54353 Mailed Apr. 20, 2012 (34 pages).
- International Search Report and Written Opinion for PCT/US12/024745 Mailed May 11, 2012 (21 pages).
- International Search Report and Written Opinion for PCT/US12/24741 Mailed Jun. 12, 2012 (12 pages).
- International Search Report and Written Opinion for PCT/US12/5499 Mailed May 29, 2012 (10 pages).
- International Search Report and Written Opinion for PCT/US2009/050931 Mailed Nov. 26, 2009 (3 pages).
- International Search Report and Written Opinion for PCT/US2013/037751 dated Aug. 22, 2013.
- International Search Report and Written Opinion for PCTUS1154353 Mailed Apr. 20, 2012 (34 pages).
- International Search Report and Written Opinion for PCTUS12024745 Mailed May 11, 2012 (21 pages).
- International Search Report and Written Opinion for PCTUS1224741 Mailed Jun. 12, 2012 (12 pages).
- International Search Report and Written Opinion for PCTUS125499 Mailed May 29, 2012 (10 pages).
- International Search Report and Written Opinion in PCT/EP2010/065188 Mailed Jan. 12, 2011 (7 pages).
- International Search Report and Written Opinion in PCT/US11/24615 Mailed Jul. 25, 2011 (37 pages).
- International Search Report and Written Opinion in PCT/US2004/010903 Mailed Dec. 20, 2004 (16 pages).
- International Search Report and Written Opinion in PCT/US2006/021286 Mailed Sep. 14, 2007 (16 pages).
- International Search Report and Written Opinion in PCT/US2007/002063 Mailed Nov. 15, 2007 (20 pages).
- International Search Report and Written Opinion mailed on Nov. 25, 2014, for International Patent Application No. PCT/US14/34037, filed Apr. 14, 2014, 13 pages.
- International Search Report for PCT/US2003/2052 dated Jun. 6, 2004.
- Sugiura et al., Effect of Channel Structure on MicroChannel Emulsification, *Langmuir* 18:5708-5712 (2002).
- Sugiura et al., Interfacial tension driven monodispersed droplet formation from microfabricated channel array *Langmuir*, 17: 5562-5566 (2001).
- Sundberg et al., Spatially-Addressable Immobilisation of Macromolecules on Solid Supports, *J. Am. Chem. Soc.*, 117:12050-12057 (1995).
- Sung et al. Chip-based microfluidic devices coupled with electrospray ionization-mass spectrometry, *Electrophoresis* 26:1783-1791 (2005).
- Suzuki et al., Random mutagenesis of thermus aquaticus DNA polymerase I: concordance of immutable sites in vivo with the crystal structure, *PNAS USA*, 93:96701-9675 (1996).
- Tabatabai and Faghri, A New Two-Phase Flow Map and Transition Boundary Accounting for Surface Tension Effects in Horizontal Miniature and Micro Tubes, *J Heat Transfer* 123:958-968 (2001).
- Tabatabai et al, Economic feasibility study of polyelectrolyte-enhanced ultrafiltration (PEUF) for water softening, *J Membrane Science* 100(3):193-207 (1995).
- Tabatabai et al., Reducing Surfactant Adsorption on Carbonate Reservoirs, *SPE Reservoir Engineering* 8(2):117-122 (1993).
- Tabatabai, Water Softening Using polyelectrolyte-enhanced ultrafiltration, *Separation Science Technology* 30 (2):211-224 (1995).
- Takayama et al., Patterning Cells and Their Environments Using Multiple Laminar Fluid Flows in Capillary Networks, *PNAS* 96:5545-5548 (1999).
- Takeuchi et al., An Axisymmetric Flow-Focusing Microfluidic Device, *Adv. Mater* 17(8):1067-1072 (2005).
- Taly et al., Droplets as Microreactors for High-Throughput Biology, *Chembiochem* 8(3):263-272 (2007).
- Tan et al., Controlled Fission of Droplet Emulsions in Bifurcating Microfluidic Channels, *Transducers Boston* (2003).
- Tan et al., Design of microfluidic channel geometries for the control of droplet volume, chemical concentration, and sorting, *Lab Chip*, 4(4): 292-298 (2004).
- Tan et al., Monodispersed microfluidic droplet generation by shear focusing microfluidic device, *Sensors and Actuators* 114:350-356 (2006).

(56)

References Cited

OTHER PUBLICATIONS

- Tan, Y.C., Microfluidic Liposome Generation from Monodisperse Droplet Emulsion—Towards the Realization of Artificial Cells, Summer Bioengineering Conference, Florida (2003).
- Tan, Y.C., Monodisperse Droplet Emulsions in Co-Flow Microfluidic Channels, Micro TAS, Lake Tahoe (2003).
- Tanaka et al., Ethanol Production from Starch by a Coimmobilized Mixed Culture System of *Aspergillus awamori* and *Zymomonas mobilis*, *Biotechnol Bioeng* XXVII:1761-1768 (1986).
- Tang et al., A multi-color fast-switching microfluidic droplet dye laser, *Lab Chip* 9:2767-2771 (2009).
- Taniguchi et al., Chemical Reactions in Microdroplets by Electrostatic Manipulation of Droplets in Liquid Media, *Lab on a Chip* 2:19-23 (2002).
- Tawfik et al., catELISA: a facile general route to catalytic antibodies, *PNAS* 90(2):373-7 (1993).
- Tawfik et al., Efficient and selective p-nitrophenyl-ester=hydrolyzing antibodies elicited by a p-nitrobenzyl phosphonate hapten, *Eur J Biochem*, 244:619-26 (1997).
- Tawfik et al., Man-made cell-like compartments for molecular evolution, *Nature Biotechnology*, 7(16):652-56 (1998).
- Tawfik, D.S. et al., 1,8-diabicyclo[5.4.0]undecane mediated transesterification of p-nitrophenyl phosphonates—a novel route to phosphono esters, *Synthesis-Stuttgart*, 10: 968-972 (1993).
- Taylor et al., Characterization of chemisorbed monolayers by surface potential measurements, *J. Phys. D. Appl. Phys.* 24:1443 (1991).
- Taylor, The formation of emulsions in definable field of flow, *Proc R Soc London A* 146(858):501-523 (1934).
- Tchagang et al., Early detection of ovarian cancer using group biomarkers, *Mol Cancer Ther* 7:27-37 (2008).
- Tencza et al., Development of a Fluorescence Polarization-Based Diagnostic Assay for Equine Infectious Anemia Virus, *J Clinical Microbiol* 38(5):1854-185 (2000).
- Terray et al., Microfluidic Control Using Colloidal Devices, *Science*, 296(5574):1841-1844 (2002).
- Terray, et al, Fabrication of linear colloidal structures for microfluidic applications, *Applied Phys Lett* 81(9):1555-1557 (2002).
- Tewhey et al., Microdroplet-based PCR amplification for large scale targeted sequencing, *Nat Biotechnol* 27 (11):1025-1031 (2009).
- Tewhey et al., Microdroplet-based PCR enrichment for large scale targeted sequencing, *Nature Biotechnology*, 2009, vol. 27 (11) p. 1025-1031.
- Theberge et al., Microdroplets in Microfluidics: An Evolving Platform for Discoveries in Chemistry and Biology, *Angew. Chem. Int. Ed* 49(34):5846-5868 (2010).
- Thompson, L.F., Introduction to Lithography, ACS Symposium Series 219:1-13, (1983).
- Thorsen et al., Dynamic pattern formation in a vesicle-generating microfluidic device, *Phys Rev Lett* 86(18):4163-4166 (2001).
- Thorsen et al., Microfluidic Large-Scale Integration, *Science* 298:580-584 (2002).
- Tice et al., Effects of viscosity on droplet formation and mixing in microfluidic channels, *Analytica Chimica Acta* 507:73-77 (2004).
- Tice et al., Formation of droplets and mixing in multiphase microfluidics at low values of the reynolds and the capillary numbers, *Langmuir* 19:9127-9133 (2003).
- Titomanlio et al., Capillary experiments of flow induced crystallization of HOPE, *AIChE Journal*, 36(1):13-18(1990).
- Tleugabulova et al., Evaluating formation and growth mechanisms of silica particles using fluorescence anisotropy decay analysis, *Langmuir* 20(14):5924-5932 (2004).
- Tokatlidis et al., Nascent chains: folding and chaperone interaction during elongation on ribosomes, *Philos Trans R Soc Lond B Biol Sci*, 348:89-95 (1995).
- Tokeshi et al., Continuous-Flow Chemical Processing on a Microchip by Combining Microunit Operations and a Multiphase Flow Network, *Anal Chem* 74(7):1565-1571 (2002).
- Tokumitsu, H. et al., Preparation of gadopentetic acid-loaded chitosan microparticles for gadolinium neutron-capture therapy of cancer by a novel emulsion-droplet coalescence technique, *Chem and Pharm Bull* 47(6):838-842 (1999).
- Tramontano, A., Catalytic antibodies, *Science* 234(4783):1566-70 (1986).
- Trindade, T., Nanocrystalline semiconductors: synthesis, properties, and perspectives, *Chem. Mat.* 13:3843-3858 (2001).
- Tripet, B. et al., Engineering a de novo-designed coiled-coil heterodimerization domain off the rapid detection, purification and characterization of recombinantly expressed peptides and proteins, *Protein Engng.*, 9:1029-42 (1996).
- Tuerk, C. and Gold, L., Systematic Evolution of Ligands by Exponential Enrichment: RNA Ligands to Bacteriophage T4 DNA Polymerase, *Science*, 249:505-10 (1990).
- Umbanhowar et al., Monodisperse Emulsion Generation via Drop Break Off in a Coflowing Stream, *Langmuir* 16 (2):347-351 (2000).
- Unger et al., Monolithic microfabricated valves and pumps by multilayer soft lithography, *Science* 288(5463):113-116 (2000).
- Utada, A. et al., Monodisperse double emulsions generated from a microcapillary device, *Science*, 308:537-541 (2005).
- Endo et al. Kinetic determination of trace cobalt by visual autocatalytic indication, *Talanta* 47:349-353 (1998).
- Endo et al., Autocatalytic decomposition of cobalt complexes as an indicator system for the determination of trace amounts of cobalt and effectors, *Analyst* 121:391-394 (1996).
- Engl, W. et al, Droplet Traffic at a Simple Junction at Low Capillary Numbers *Physical Review Letters*, 2005, vol. 95,208304.
- Eow et al., Electrocoalesce-separators for the separation of aqueous drops from a flowing dielectric viscous liquid, *Separation and Purification Tech* 29:63-77 (2002).
- Eow et al., Electrostatic enhancement of coalescence of water droplets in oil: a review of the technology, *Chemical Engineering Journal* 85:357-368 (2002).
- Eow et al., Motion, deformation and break-up of aqueous drops in oils under high electric field strengths, *Chemical Eng Proc* 42:259-272 (2003).
- Eow et al., The behavior of a liquid-liquid interface and drop-interface coalescence under the influence of an electric field, *Colloids and Surfaces A: Physiochem. Eng. Aspects* 215:101-123 (2003).
- Eow, et al. Electrostatic and hydrodynamic separation of aqueous drops in a flowing viscous oil, *Chemical Eng Proc* 41:649-657 (2002).
- European Office Action dated Apr. 29, 2014 for EP 08165420.4.
- European Search Report for EP 13165665.4 mailed Nov. 22, 2013, 4 pages.
- European Search Report for EP 13165667.0 mailed Nov. 22, 2013, 4 pages.
- European Search Report for EP Application No. 13165665 with the date of the completion of the search Nov. 15, 2013 (4 pages).
- European Search Report for EP Application No. 13165667 with the date of the completion of the search Nov. 15, 2013 (4 pages).
- Extended European Search Report for EP 10181911.8 mailed Jun. 1, 2011 (7 pages).
- Extended European Search Report for EP 10184514.7 mailed Dec. 20, 2010 (5 pages).
- Extended European Search Report for EP 10196179 mailed May 2, 2014 (10 pages).
- Extended European Search Report for EP 10196339 mailed May 2, 2014 (9 pages).
- Faca et al., A mouse to human search for plasma proteome changes associated with pancreatic tumor development, *PLoS Med* 5(6):e123 (2008).
- Fahy et al., Self-sustained sequence replication (3SR): an isothermal transcription-based amplification system alternative to PCR, *PCR Methods Appl* 1:25-33 (1991).
- Fan and Harrison, Micromachining of capillary electrophoresis injectors and separators on glass chips and evaluation of flow at capillary intersections, *Anal Chem* 66:177-184 (1994).
- Fastrez, J., In vivo versus in vitro screening or selection for catalytic activity in enzymes and abzymes, *Mol Biotechnol* 7(1):37-55 (1997).

(56)

References Cited

OTHER PUBLICATIONS

- Fettinger et al., Stacked modules for micro flow systems in chemical analysis: concept and studies using an enlarged model, *Sens Actuat B*, 17:19-25 (1993).
- Fiedler et al., Dielectrophoretic sorting of particles and cells in a microsystem, *Anal Chem* 70(9):1909-1915 (1998).
- Field, J. et al., Purification of a RAS-responsive adenylyl cyclase complex from *Saccharomyces cerevisiae* by use of an epitope addition method. *Mol Cell Biol*, 8: 2159-2165 (1988).
- Fields, S. and Song, O., A novel genetic system to detect protein-protein interactions, *Nature* 340(6230):245-6 (1989).
- Filella et al., TAG-72, CA 19.9 and CEA as tumor markers in gastric cancer, *Acta Oncol.* 33(7):747-751 (1994).
- Finch, C.A., Encapsulation and controlled release, *Spec Publ R Soc Chem*, 138:35 (1993).
- Finch, C.A., Industrial Microencapsulation: Polymers for Microcapsule Walls, 1-12 in *Encapsulation and Controlled Release*, Woodhead Publishing (1993).
- Fire & Xu, Rolling replication of short DNA circles, *PNAS* 92(10):4641-5 (1995).
- Firestine, S.M. et al., Using an AraC-based three hybrid system to detect biocatalysts in vivo, *Nat Biotechnol* 18: 544-547 (2000).
- Fisch et al., A strategy of exon shuffling for making large peptide repertoires displayed on filamentous bacteriophage, *PNAS* 93:7761-6 (1996).
- Fisher et al., Cell Encapsulation on a Microfluidic Platform, The Eighth International Conference on Miniaturised Systems for Chemistry and Life Sciences, MicroTAS, Sep. 26-30, 2004, Malmo, Sweden.
- Fletcher et al., Micro reactors: principles and applications in organic synthesis, *Tetrahedron* 58:4735-4757 (2002).
- Fluri et al., Integrated capillary electrophoresis devices with an efficient postcolumn reactor in planar quartz and glass chips, *Anal Chem* 68:4285-4290 (1996).
- Fornusek, L. et al., Polymeric microspheres as diagnostic tools for cell surface marker tracing, *Crit Rev Ther Drug Carrier Syst*, 2:137-74 (1986).
- Fowler, Enhancement of Mixing by Droplet-Based Microfluidics, *Int Conf MEMS* 97-100 (2002).
- Freese, E., The specific mutagenic effect of base analogues on Phage T4, *J Mol Biol*, 1: 87 (1959).
- Frenz et al., Reliable microfluidic on-chip incubation of droplets in delay-lines, *Lab on a Chip* 9:1344-1348 (2008).
- Fu et al., A microfabricated fluorescence-activated cell sorter, *Nature Biotechnology*, 17(11):1109-1111 (1999).
- Fu et al., An Integrated Microfabricated Cell Sorter, *Anal. Chem.*, 74: 2451-2457 (2002).
- Fulton et al., Advanced multiplexed analysis with the FlowMetrix system, *Clin Chem* 43:1749-1756 (1997).
- Fulwyler, Electronic Separation of Biological Cells by Volume, *Science* 150(3698):910-911 (1965).
- Fungi (Wikipedia.com accessed Jun. 3, 2013).
- Gallarate et al., On the stability of ascorbic acid in emulsified systems for topical and cosmetic use, *Int J Pharm* 188 (2):233-241 (1999).
- Ganan-Calvo, A.M., Perfectly Monodisperse Microbubbling by Capillary Flow Focusing, *Phys Rev Lett* 87(27): 274501-1-4 (2001).
- Ganan-Calvo, Generation of Steady Liquid Microthreads and Micron-Sized Monodisperse Sprays and Gas Streams, *Phys Rev Lett* 80(2):285-288 (1998).
- Garcia-Ruiz et al. A super-saturation wave of protein crystallization, *J. Crystal Growth*, 232:149-155(2001).
- Garcia-Ruiz et al., Investigation on protein crystal growth by the gel acupuncture method, *Acta, Cryst.*, 1994, D50, 99. pp. 484-490.
- Garstecki, et al., Formation of monodisperse bubbles in a microfluidic flow-focusing device, *Appl Phys Lett* 85 (13):2649-2651 (2004).
- Gasparlin et al., The structure elucidation of semisolid w/o emulsion systems containing silicone surfactant, *Intl J Pharm*, 107:51-6 (1994).
- Vainshtein et al., Peptide rescue of an N-terminal truncation of the stoffel fragment of Taq DNA polymerase, *Protein Science*, 5:1785-92 (1996).
- Van Bockstaele et al., Prognostic markers in chronic lymphocytic leukemia: a comprehensive review, *Blood Rev* 23 (1):25-47 (2009).
- Van Dilla et al., Cell Microfluorometry: A Method for Rapid Fluorescence Measurement, *Science* 163(3872):1213-1214 (1969).
- Van Dilla et al., The fluorescent cell photometer: a new method for the rapid measurement of biological cells stained with fluorescent dyes, Annual Report of the Los Alamos Scientific Laboratory of the University of California (Los Alamos, NM), Biological and Medical Research Group (H-4) of the Health Division, Compiled by D. G. Ott, pp. 100-105, distributed Jan. 23, 1968.
- Vanhooke et al., Three-dimensional structure of the zinc-containing phosphotriesterase with the bound substrate analog diethyl 4-methylbenzylphosphonate, *Biochemistry* 35:6020-6025 (1996).
- Varga, J.M. et al., Mechanism of allergic cross-reactions—I. Multispecific binding of ligands to a mouse monoclonal anti-DNP IgE antibody. *Mol Immunol* 28(6), 641-54 (1991).
- Vary, A homogeneous nucleic acid hybridization assay based on strand displacement, *Nucl Acids Res* 15 (17):6883-6897 (1987).
- Venkateswaran et al., Production of Anti-Fibroblast Growth Factor Receptor Monoclonal Antibodies by in Vitro Immunization, *Hybirdoma*, 11(6):729-739 (1992).
- Venter et al., The sequence of the human genome, *Science* 291(5507):1304-51 (2001).
- Viruses (Wikipedia.com, accessed Nov. 24, 2012).
- Vogelstein et al., Digital PCR, *PNAS* 96(16):9236-9241 (1999).
- Voss, E.W., Kinetic measurements of molecular interactions by spectrofluorometry, *J Mol Recognit*, 6:51-58 (1993).
- Wahler, D. et al., Novel methods for biocatalyst screening. *Curr Opin Chem Biol*, 5: 152-158 (2001).
- Walde, P. et al., Oparin's reactions revisited: enzymatic synthesis of poly(adenylic acid) in micelles and self-reproducing vesicles. *J Am Chem Soc*, 116: 7541-7547 (1994).
- Walde, P. et al., Spectroscopic and kinetic studies of lipases solubilized in reverse micelles, *Biochemistry*, 32 (15):4029-34 (1993).
- Walde, P. et al., Structure and activity of trypsin in reverse micelles, *Eur J Biochem*, 173(2):401-9 (1988).
- Walker et al., Isothermal in vitro amplification of DNA by a restriction enzyme/DNA polymerase system, *PNAS* 89 (1):392-6 (1992).
- Walker et al., Strand displacement amplification—an isothermal, in vitro DNA amplification technique, *Nucleic Acid Res*, 20(7):1691-6 (1992).
- Wang et al., DEP actuated nanoliter droplet dispensing using feedback control, *Lab on a Chip* 9:901-909 (2008).
- Wang et al., Preparation of Titania Particles Utilizing the Insoluble Phase Interface in a MicroChannel Reactor, *Chemical Communications* 14:1462-1463 (2002).
- Wang, A.M. et al., Quantitation of mRNA by the polymerase chain reaction. *Proc natl Acad Sci USA* 86(24), 9717-21 (1989).
- Wang, G.T. et al., Design and synthesis of new fluorogenic HIV protease substrates based on resonance energy transfer, *Tetrahedron Lett.*, 31:6493 (1990).
- Wang, Jun, et al., Quantifying EGFR Alterations in the Lung Cancer Genome with Nanofluidic Digital PCR Arrays, *Clinical Chemistry* 56:4 (2010).
- Warburton, B., Microcapsules for Multiple Emulsions, Encapsulation and Controlled Release, *Spec Publ R Soc Chem*, 35-51 (1993).
- Wasserman et al., Structure and reactivity of allyl-siloxane monolayers formed by reaction of allyltrichlorosilanes on silicon substrates, *Langmuir* 5:1074-1087 (1989).
- Weaver, Suzanne, et al., Taking qPCR to a higher level: Analysis of CNV reveals the power of high throughput qPCR to enhance quantitative resolution, *Methods* 50, 271-276 (2010).
- Weil et al., Selective and accurate initiation of transcription at the Ad2 major late promoter in a soluble system dependent on purified RNA polymerase II and DNA, *Cell*, 18(2):469-84 (1979).
- Werle et al., Convenient single-step, one tube purification of PCR products for direct sequencing, *Nucl Acids Res* 22 (20):4354-4355 (1994).

(56)

References Cited

OTHER PUBLICATIONS

- Wetmur et al., Molecular haplotyping by linking emulsion PCR: analysis of paraoxonase 1 haplotypes and phenotypes, *Nucleic Acids Res* 33(8):2615-2619 (2005).
- Wick et al., Enzyme-containing liposomes can endogenously produce membrane-constituting lipids, *Chem Biol* 3 (4):277-85 (1996).
- Widersten and Mannervik, Glutathione Transferases with Novel Active Sites Isolated by Phage Display from a Library of Random Mutants, *J Mol Biol* 250(2):115-22 (1995).
- Wiggins et al., Foundations of chaotic mixing, *Philos Transact A Math Phys Eng Sci* 362(1818):937-70 (2004).
- Williams et al., Amplification of complex gene libraries by emulsion PCR, *Nature Methods* 3(7):545-550 (2006).
- Williams et al., Methotrexate, a high-affinity pseudosubstrate of dihydrofolate reductase, *Biochemistry*, 18(12):2567-73 (1979).
- Wilson, D.S. and Szostak, J.W., In vitro selection of functional nucleic acids, *Ann. Rev. Biochem.* 68: 611-647 (1999).
- Winter et al., Making antibodies by phage display technology, *Annu Rev Immunol* 12:433-55 (1994).
- Wittrup, K.D., Protein engineering by cell-surface display. *Curr Opin Biotechnology*, 12: 395-399 (2001).
- Wittwer, C.T., et al., Automated polymerase chain reaction in capillary tubes with hot air, *Nucleic Acids Res.*, 17(11) 4353-4357 (1989).
- Wittwer, Carl T., et al., Minimizing the Time Required for DNA Amplification by Efficient Heat Transfer to Small Samples, *Anal. Biochem.*, 186, 328-331 (1990).
- Wolff et al., Integrating advanced functionality in a microfabricated high-throughput fluorescent-activated cell sorter, *Lab Chip*, 3(1): 22-27 (2003).
- Woolley, Adam T. and Mathies, Richard A., Ultra-high-speed DNA fragment separations using microfabricated capillary array electrophoresis chips, *Proc. Natl. Acad. Sci. USA*, 91, 11348-11352 (Nov. 1994).
- Woolley, Adam T., et al., Functional Integration of PCR Amplification and Capillary Electrophoresis in a Microfabricated DNA Analysis Device, *Anal. Chem.* 68, 4081-4086 (Dec. 1, 1996).
- Written Opinion for PCT/US2004/027912 dated Jan. 26, 2005, 6 pages.
- Written Opinion for PCT/US2006/001938 dated May 31, 2006, 8 pages.
- Wronski et al., Two-color, fluorescence-based microplate assay for apoptosis detection. *Biotechniques*, 32:666-668 (2002).
- Wu et al., The ligation amplification reaction (LAR)—amplification of specific DNA sequences using sequential rounds of template-dependent ligation, *Genomics* 4(4):560-9 (1989).
- Wyatt et al., Synthesis and purification of large amounts of RNA oligonucleotides, *Biotechniques* 11(6):764-9 (1991).
- Xia and Whitesides, Soft Lithography, *Angew. Chem. Int. Ed.* 37:550-575 (1998).
- Xia and Whitesides, Soft Lithography, *Ann. Rev. Mat. Sci.* 28:153-184 (1998).
- Xu et al., Design of 240, 000 orthogonal 25mer DNA barcode probes, *PNAS*, Feb. 17, 2009, 106(7) p. 2289-2294.
- Cortesi et al., Production of lipospheres as carriers for bioactive compounds, *Biomaterials*, 23(11): 2283-2294 (2002).
- Courrier et al., Reverse water-in-fluorocarbon emulsions and microemulsions obtained with a fluorinated surfactant, *Colloids and Surfaces A: Physicochem. Eng. Aspects* 244:141-148 (2004).
- Craig, D. et al., Fluorescence-based enzymatic assay by capillary electrophoresis laser-induced fluorescence detection for the determination of a few alpha-galactosidase molecules, *Anal. Biochem.* 226:147 (1995).
- Creagh, A.L. et al., Structural and catalytic properties of enzymes in reverse micelles, *Enzyme Microb Technol* 15 (5):383-92 (1993).
- Crosland-Taylor, A Device for Counting Small Particles suspended in a Fluid through a Tube, *Nature* 171:37-38 (1953).
- Crowley, J. M., Electrical breakdown of bimolecular lipid membranes as an electromechanical instability, *Biophys J.* 13 (7):711-724 (1973).
- Cull, M.G. et al., Screening for receptor ligands using large libraries of peptides linked to the C terminus of the lac repressor, *PNAS* 89:1865-9 (1992).
- Curran, D.P., Strategy-level separations in organic synthesis: from planning to practice. *Angew Chem Int Ed*, 37:1174-11-96 (1998).
- Czarnik, A.W., Encoding methods for combinatorial chemistry, *Curr Opin Chem Biol* 1:60-66 (1997).
- Dankwardt et al., Combinatorial synthesis of small-molecule libraries using 3-amino-5-hydroxybenzoic acid, 1:113-120 (1995).
- Davis, J.A. et al., Deterministic hydrodynamics: Taking blood apart, *PNAS* 103:14779-14784 (2006).
- Davis, S.S. et al., Multiple emulsions as targetable delivery systems, *Methods in Enzymology*, 149:51-64 (1987).
- de Gans, B.J. et al., Inkjet printing of polymers: state of the art and future developments, *Advanced materials*, 16: 203-213 (2004).
- De Wildt, Ruud, et al., Isolation of receptor-ligand pairs by capture of long-lived multivalent interaction complexes, *Proceedings of the National Academy of Sciences of the United States*, 99, 8530-8535 (2002).
- De-Bashan, L. E. et al., Removal of ammonium and phosphorus ions from synthetic wastewater by the microalgae *Chlorella vulgaris* coimmobilized in alginate beads with the microalgae growth-promoting bacterium *Azospirillum brasilense*, *Water Research* 36:2941-2948 (2002).
- Delagrave, S. et al., Red-shifted excitation mutants of the green fluorescent protein, *Biotechnology* 13(2):151-4 (1995).
- DelRaso, In vitro methodologies for enhanced toxicity testing, *Toxicol. Lett.* 68:91-99 (1993).
- Demartis et al., A strategy for the isolation of catalytic activities from repertoires of enzymes displayed on phage, *J. Mol. Biol* 286:617-633 (1999).
- Dickinson, E., Emulsions and droplet size control, Wedlock, D.J., Ed., in *Controlled Particle Droplet and Bubble Formulation*, Butterworth-Heinemann, 191-257 (1994).
- DiMatteo, et al., Genetic conversion of an SMN2 gene to SMN1: A novel approach to the treatment of spinal muscular atrophy, *Exp Cell Res.* 314(4):878-886 (2008).
- Dinsmore et al., Colioidosomes: Selectively Permeable Capsules Composed of Colloidal Particles, *Science* 298 (5595):1006-1009. (2002).
- Dittrich et al., A new embedded process for compartmentalized cell-free protein expression and on-line detection in microfluidic devices, *Chembiochem* 6(5):811-814 (2005).
- Doi et al., In vitro selection of restriction endonucleases by in vitro compartmentalization, *Nucleic Acids Res*, 32(12): e95 (2004).
- Doi, N. and Yanagawa, H. Stable: protein-DNA fusion system for screening of combinatorial protein libraries in vitro, *FEBS Lett.*, 457: 227-230 (1999).
- Doman, T.N. et al., Molecular docking and high-throughput screening for novel inhibitors of protein tyrosine phosphatase-1B, *J Med Chem*, 45: 2213-2221 (2002).
- Domling A., Recent advances in isocyanide-based multicomponent chemistry, *Curr Opin Chem Biol*, 6(3):306-13 (2002).
- Domling and Ugi, Multicomponent Reactions with Isocyanides, *Angew Chem Int Ed* 39(18):3168-3210 (2000).
- Dove et al., In Brief, *Nature Biotechnology* 20:1213 (2002).
- Dower et al., High efficiency transformation of *E. coli* by high voltage electroporation, *Nucleic Acids Res* 16:6127-6145 (1988).
- Dressman et al., Transforming single DNA molecules into fluorescent magnetic particles for detection and enumeration of genetic variations, *PNAS* 100:8817-22 (2003).
- Dreyfus et al., Ordered and disordered patterns in two phase flows in microchannels, *Phys Rev Lett* 90 (14):144505-1-144505-4 (2003).
- Drmanac et al., Sequencing by hybridization: towards an automated sequencing of one million M13 clones arrayed on membranes, *Electrophoresis* 13:566-573 (1992).
- Du, Wenbin, et al., SlipChip, *Lab Chip*, 2009, 9, 2286-2292.
- Dubertret et al., In vivo imaging of quantum dots encapsulated in phospholipid micelles, *Science*, 298: 1759-1762 (2002).
- Duffy et al., Rapid Prototyping of Microfluidic Systems and Polydimethylsiloxane, *Anal Chem* 70:474-480 (1998).

(56)

References Cited

OTHER PUBLICATIONS

Duggleby, R. G. Analysis of Enzyme Progress Curves by Nonlinear Regression, Pt D. Academic Press 249:61-90 (1995).

Duggleby, R. G. Enzyme Kinetics and Mechanisms, Pt D. Academic Press 249:61-90 (1995).

Dumas, D.P., Purification and properties of the phosphotriesterase from *Pseudomonas diminuta*, J Biol Chem 264: 19659-19665 (1989).

Eckert and Kunkel, DNA polymerase fidelity and the polymerase chain reaction, Genome Res 1:17-24 (1991).

Edd et al., Controlled encapsulation of single-cells into monodisperse picolitre drops, Lab Chip 8(8):1262-1264 (2008).

Edel, Joshua B. et al., Microfluidic Routes to the Controlled Production of Nanoparticles, Chemical Communications, 1136-1137 (2002).

Edris et al., Encapsulation of orange oil in a spray dried double emulsion, Nahrung/Food, 45(2):133-137 (2001).

Effenhauser et al., Glass chips for high-speed capillary electrophoresis separations with submicrometer plate heights, Anal Chem 65:2637-2642 (1993).

Eggers, Jens et al., Coalescence of Liquid Drops, J. Fluid Mech., 401:293-310 (1999).

Ehrig, T. et al., Green-fluorescent protein mutants with altered fluorescence excitation spectra, Febs Lett, 367 (2):163-66 (1995).

Eigen et al., hypercycles and compartments: compartments assists—but does not replace—hypercyclic organization of early genetic information, J Theor Biol, 85:407-11 (1980).

Eigen et al., The hypercycle: coupling of RNA and protein biosynthesis in the infection cycle of an RNA bacteriophage, Biochemistry, 30:11005-18 (1991).

Eigen, Wie entsteht information Prinzipien der selbstorganisation in der biologie, Berichte der punsen-gesellschaft fur physikalische chemi, 80:1059-81 (1976).

Ellington and Szostak, In vitro selection of RNA molecules that bind specific ligands, Nature, 346:818-822 (1990).

Ellman et al., Biosynthetic method for introducing unnatural amino acids site-specifically into proteins, Methods Enzymol, 202:301-36 (1991).

* cited by examiner

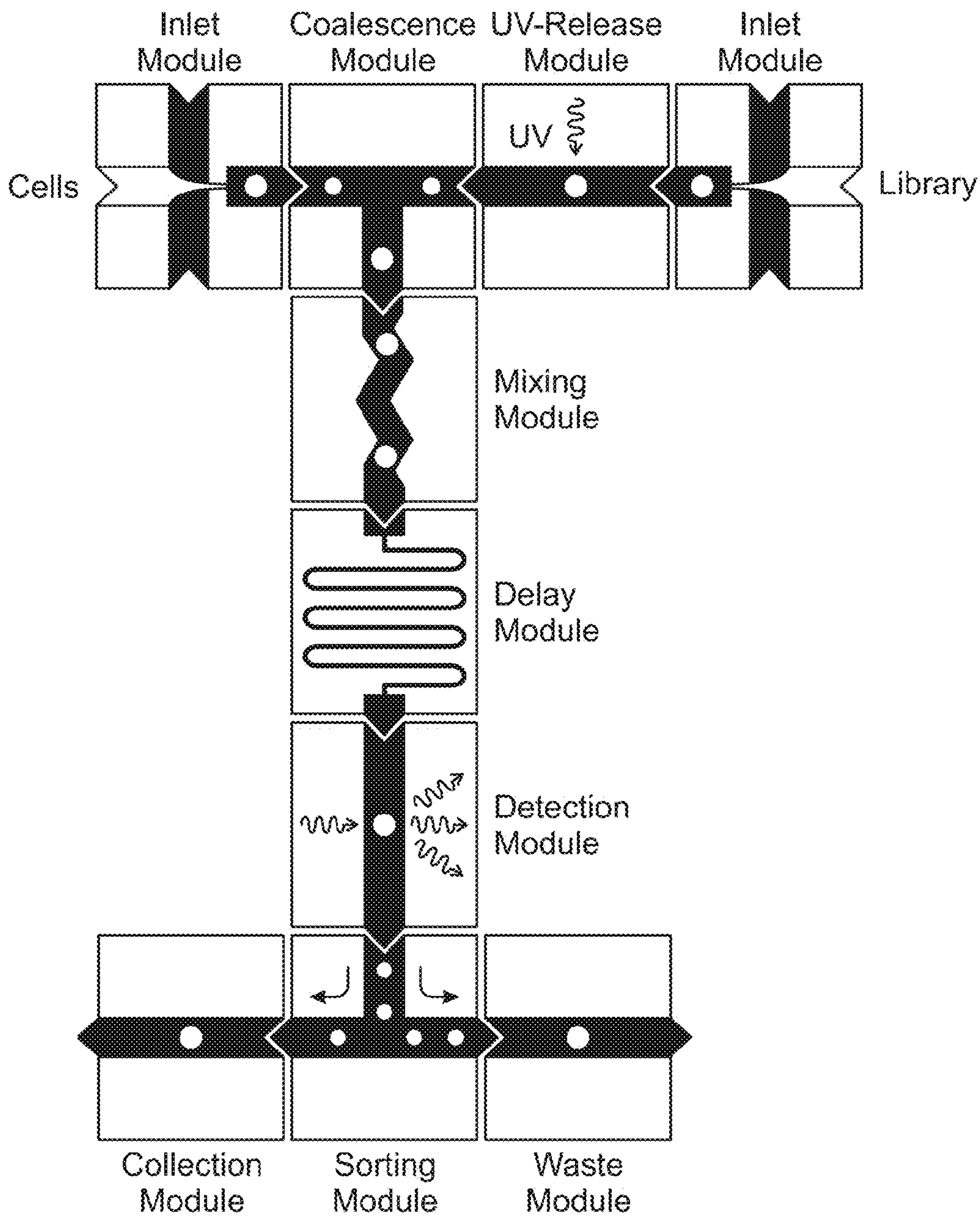


FIG. 1

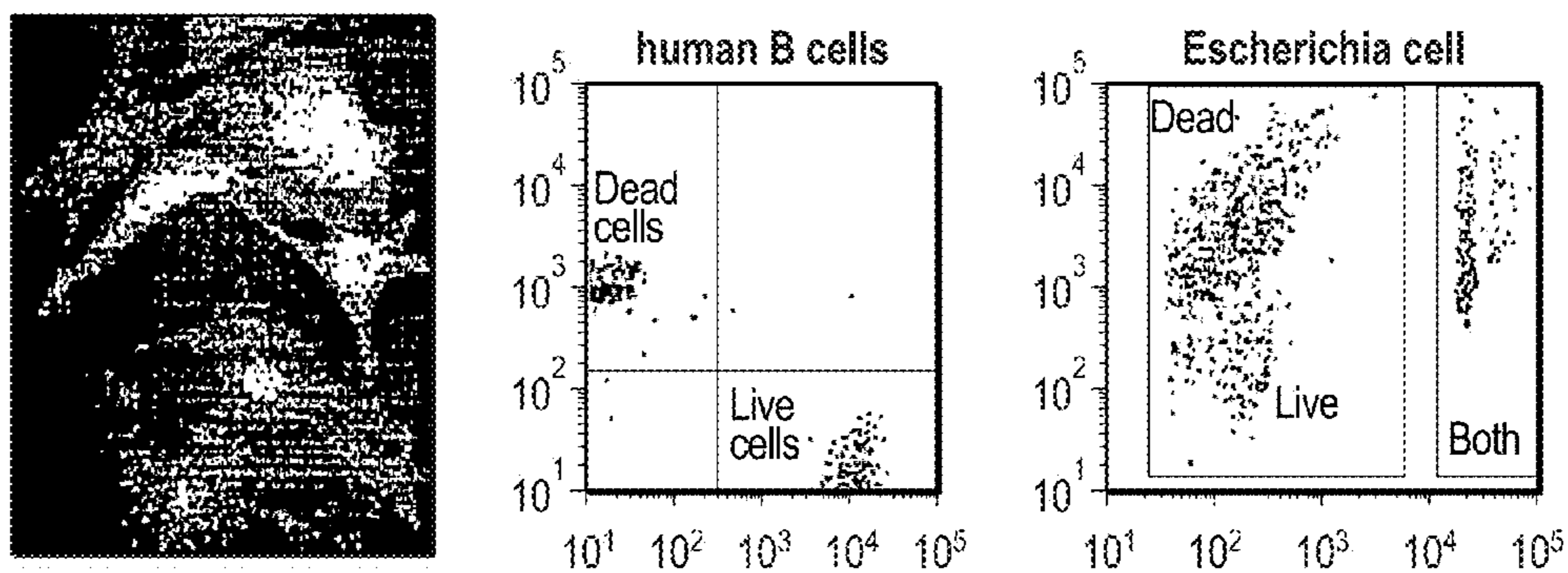


FIG. 2

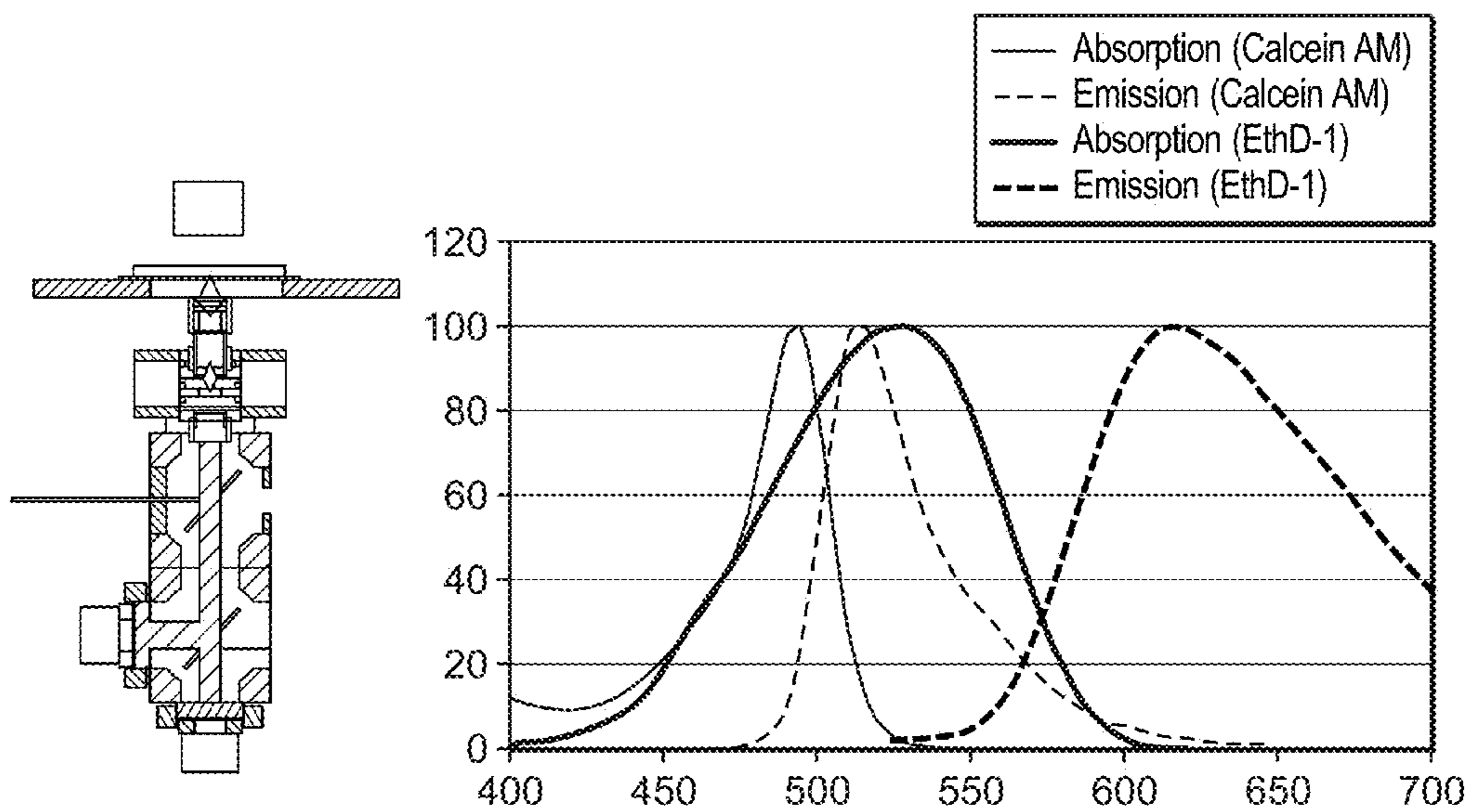


FIG. 3

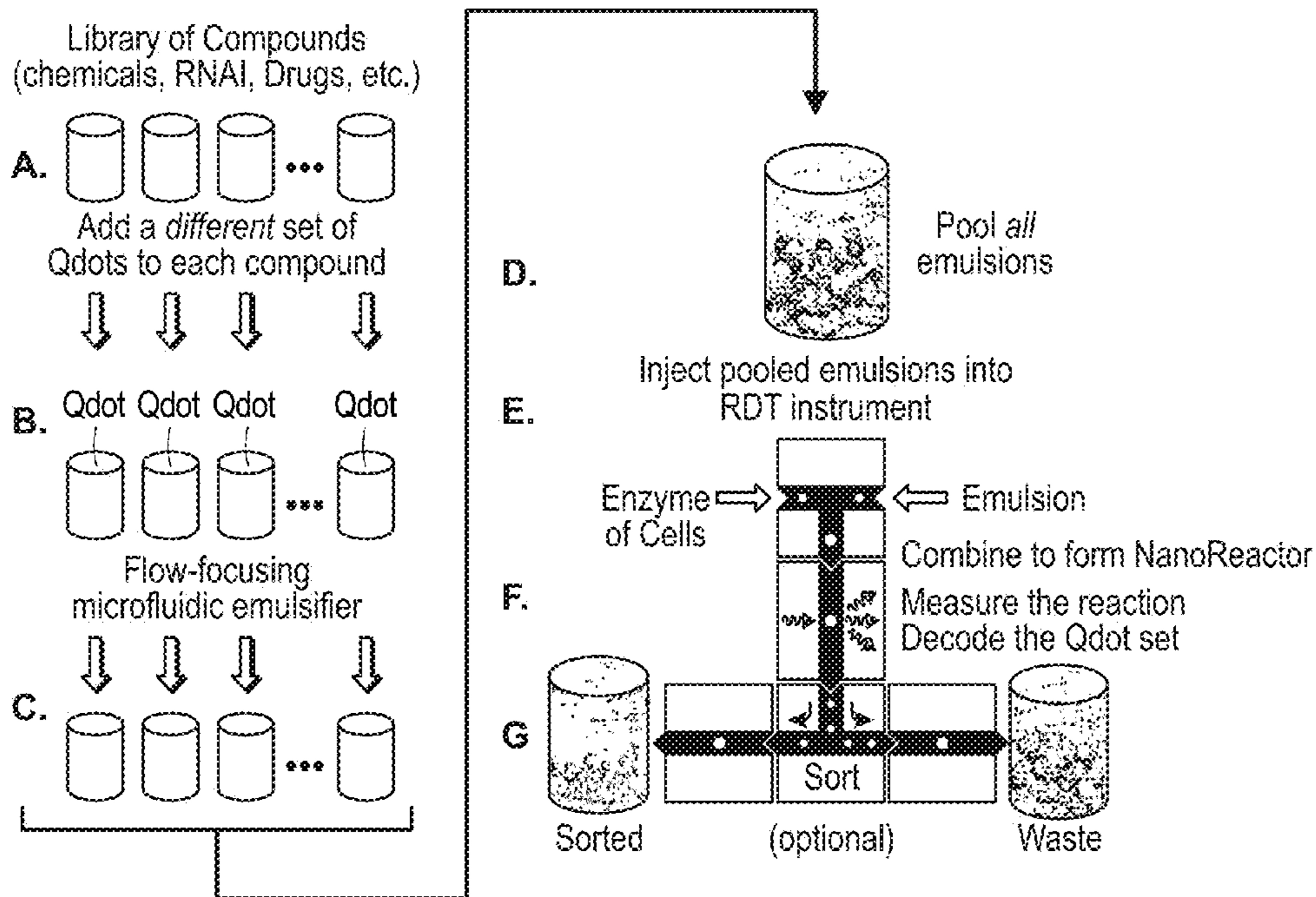


FIG. 4

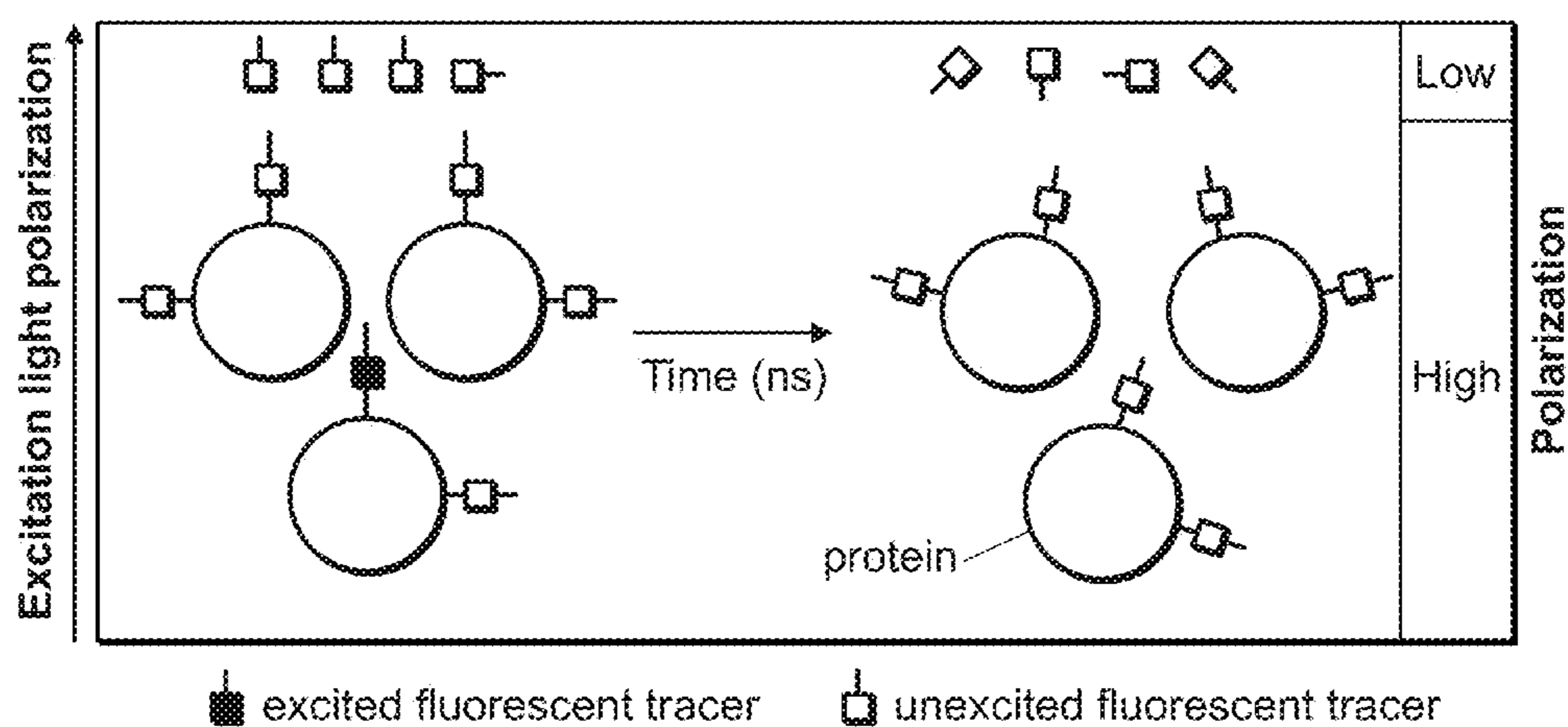


FIG. 5

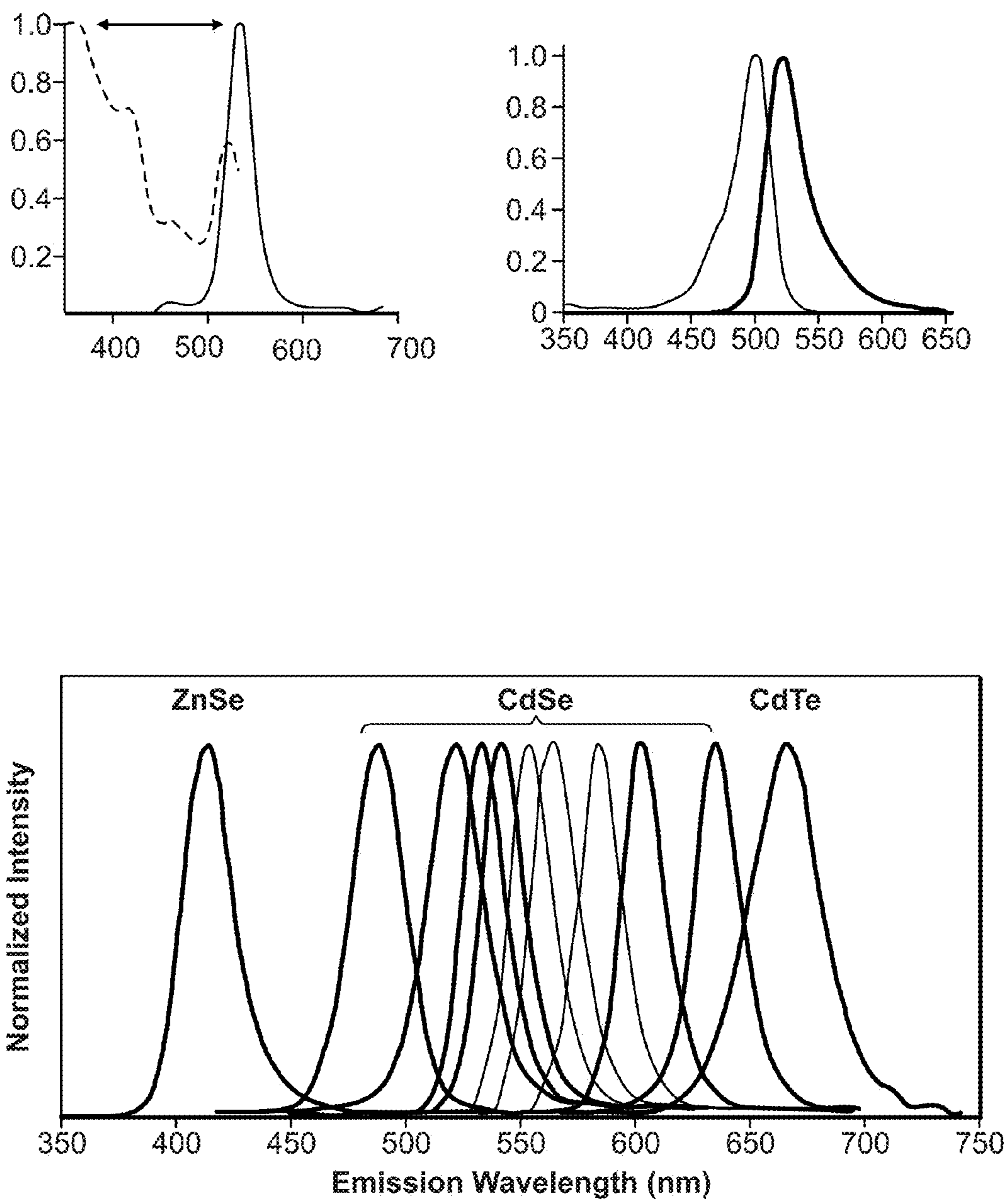


FIG. 6

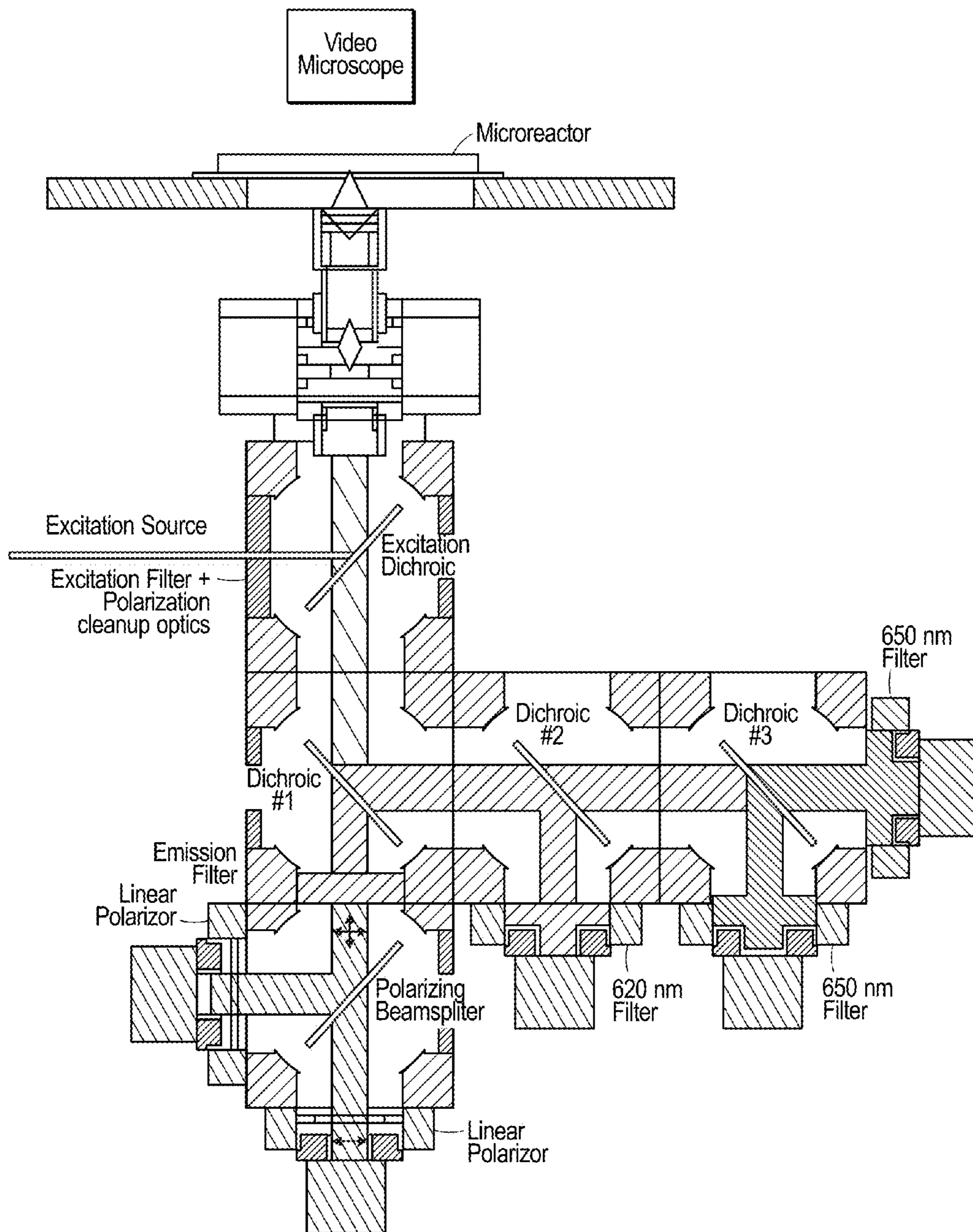


FIG. 7

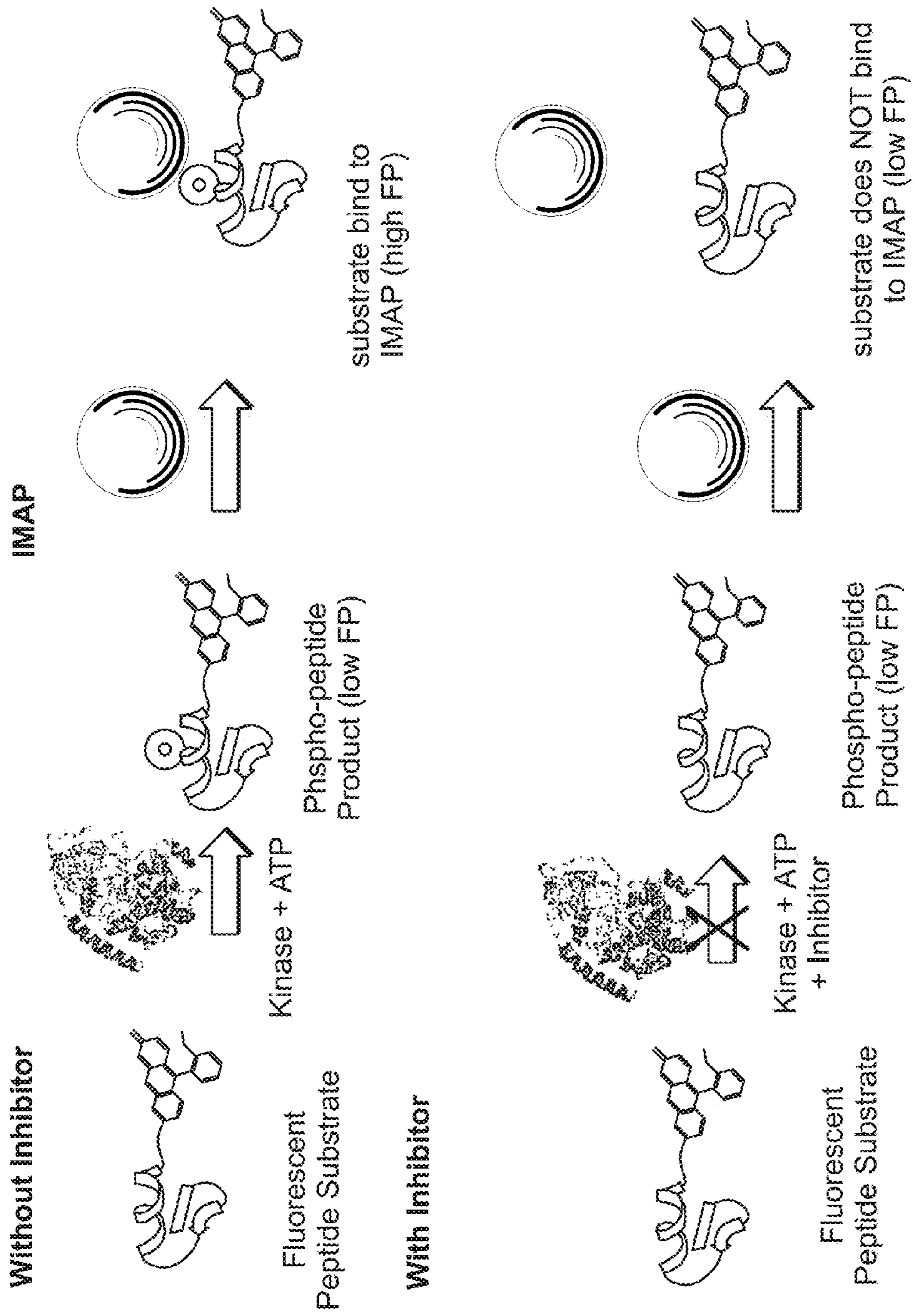


FIG. 8

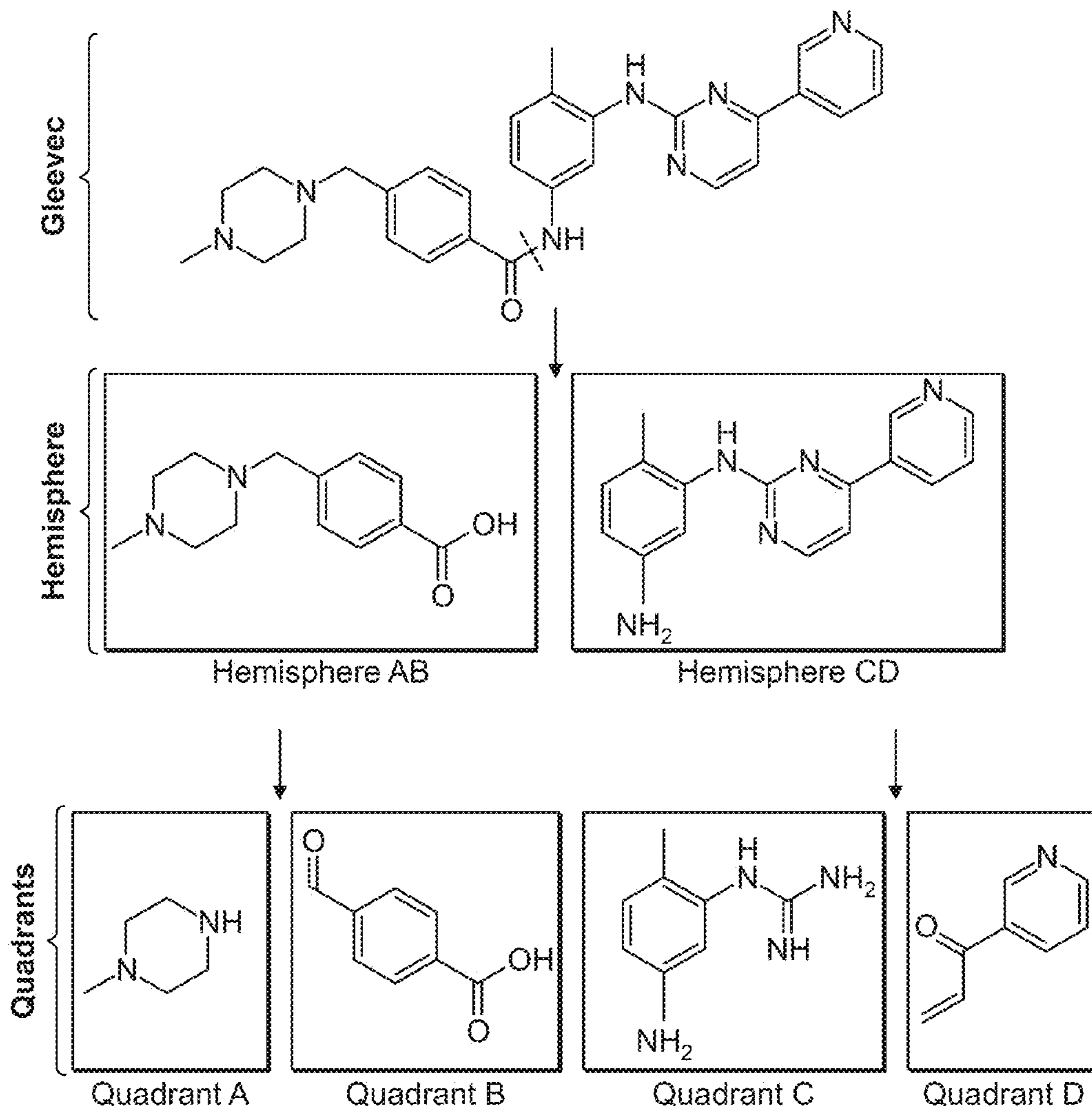


FIG. 9

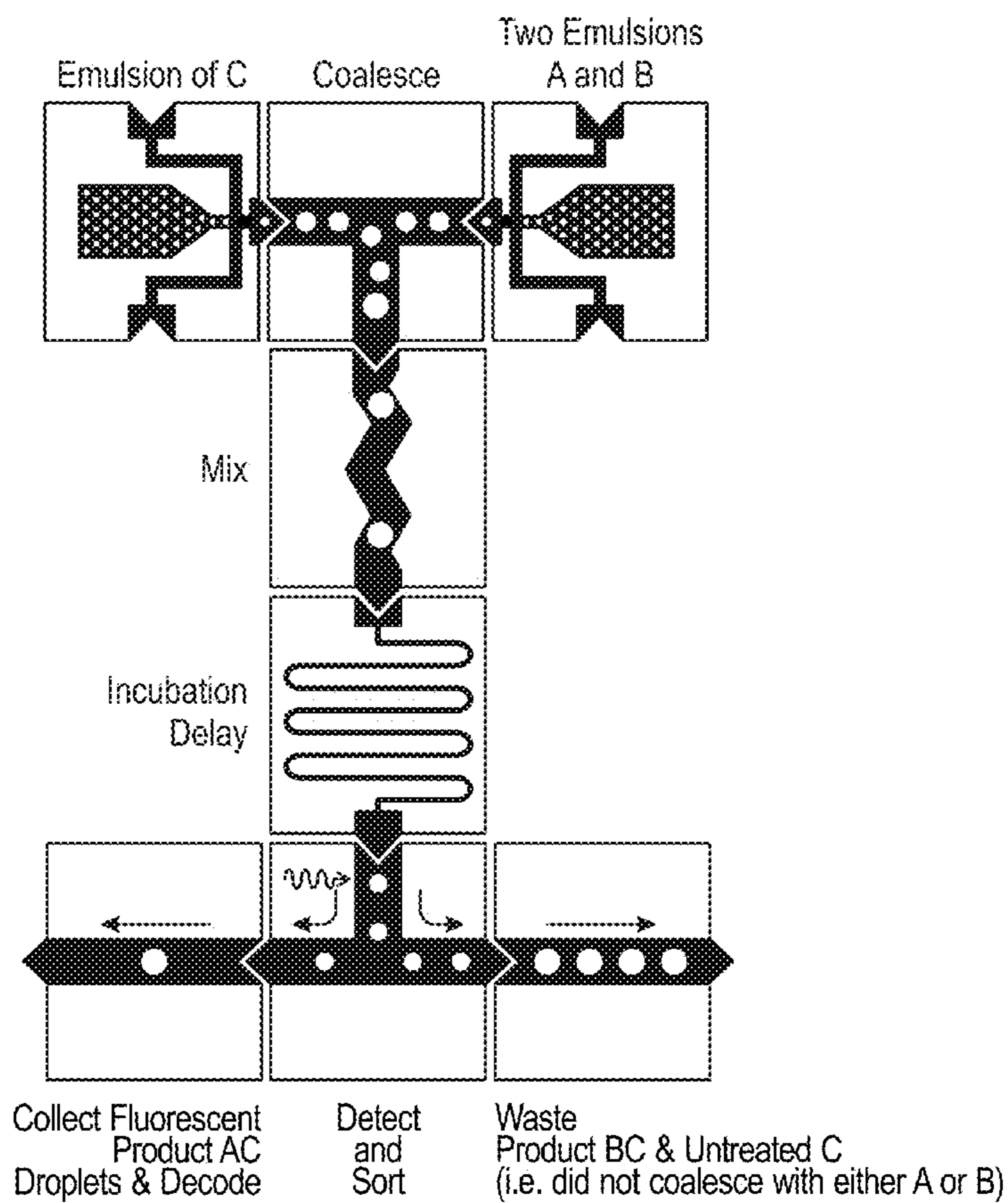
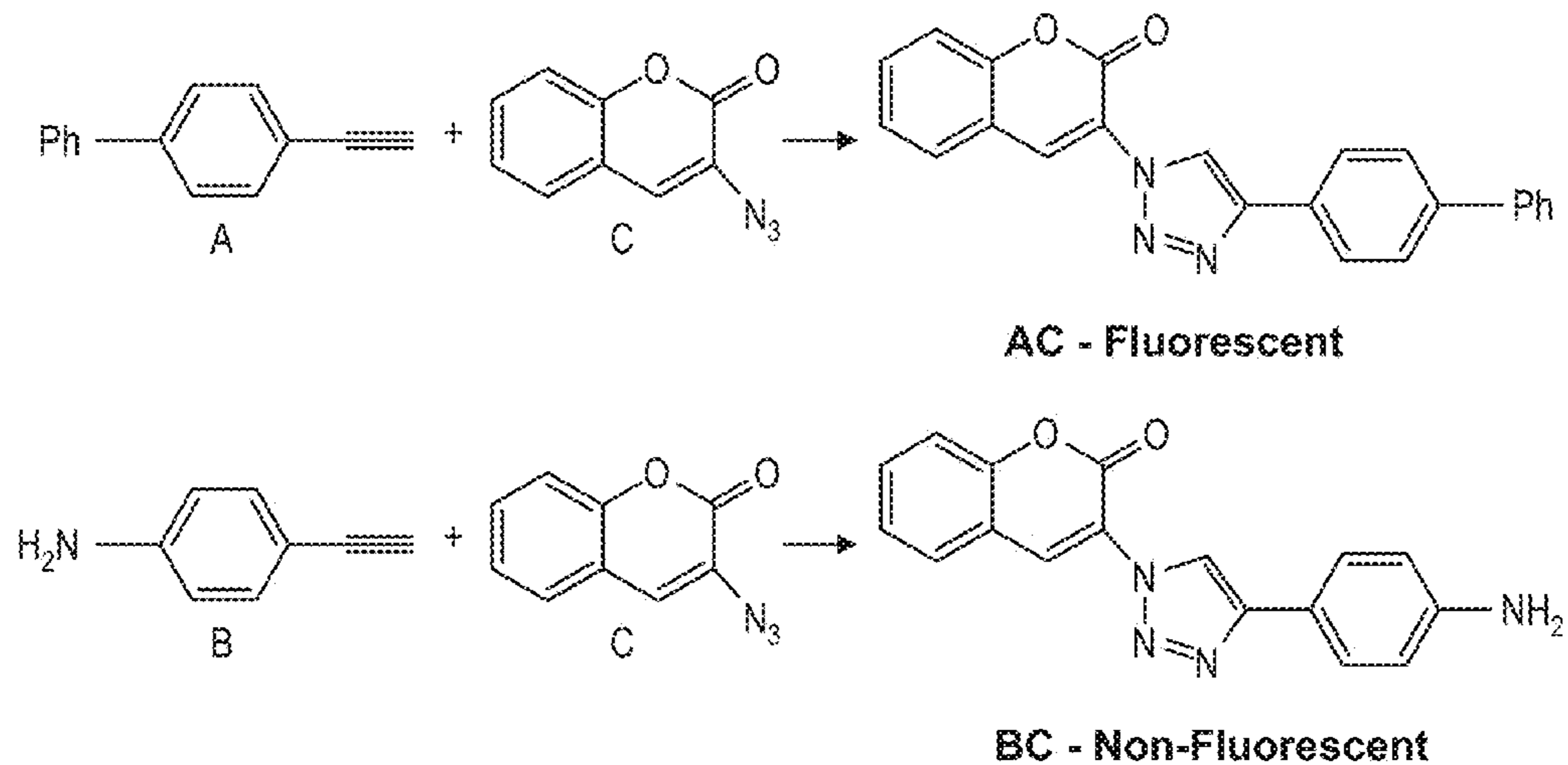


FIG. 10

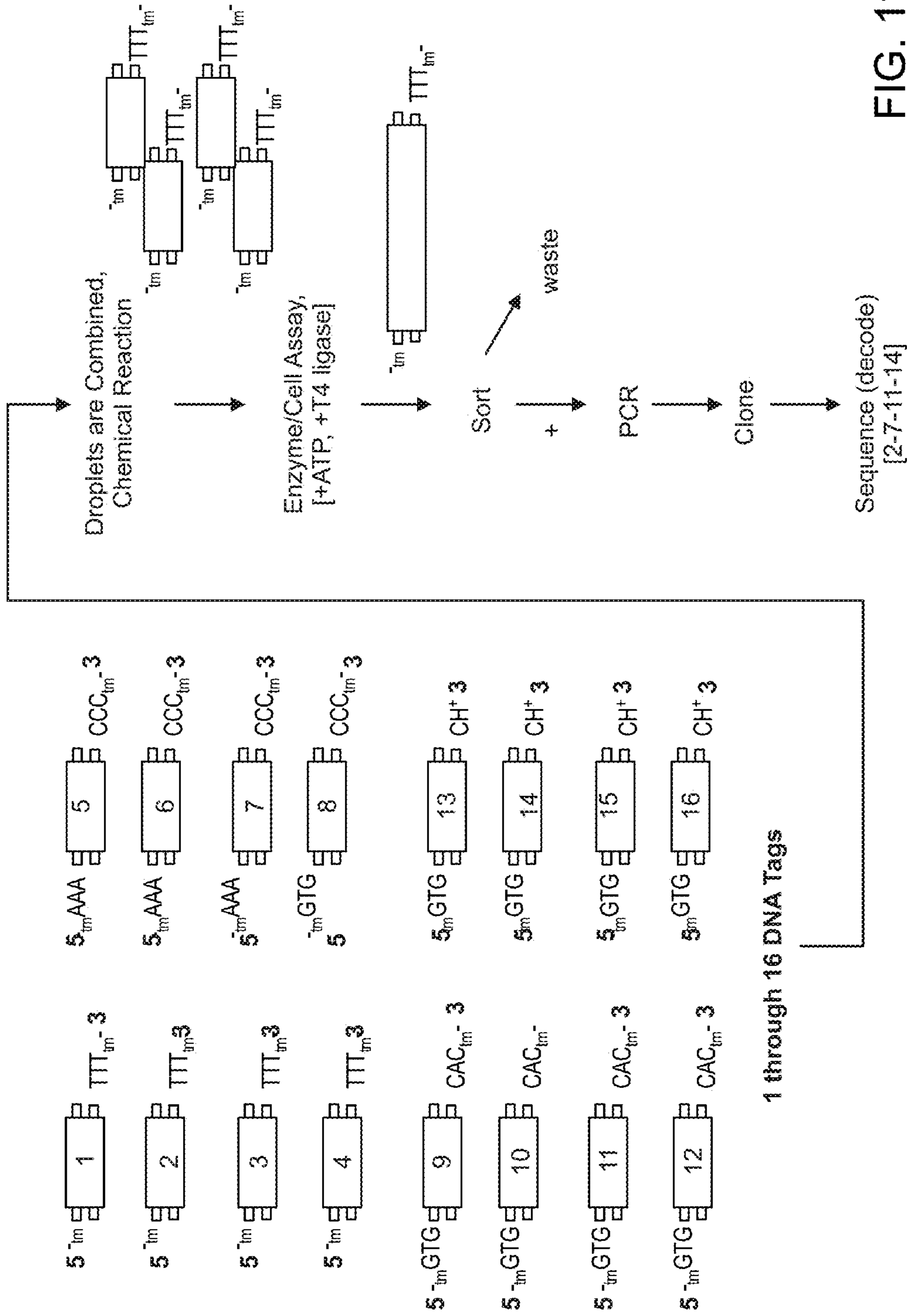


FIG. 11

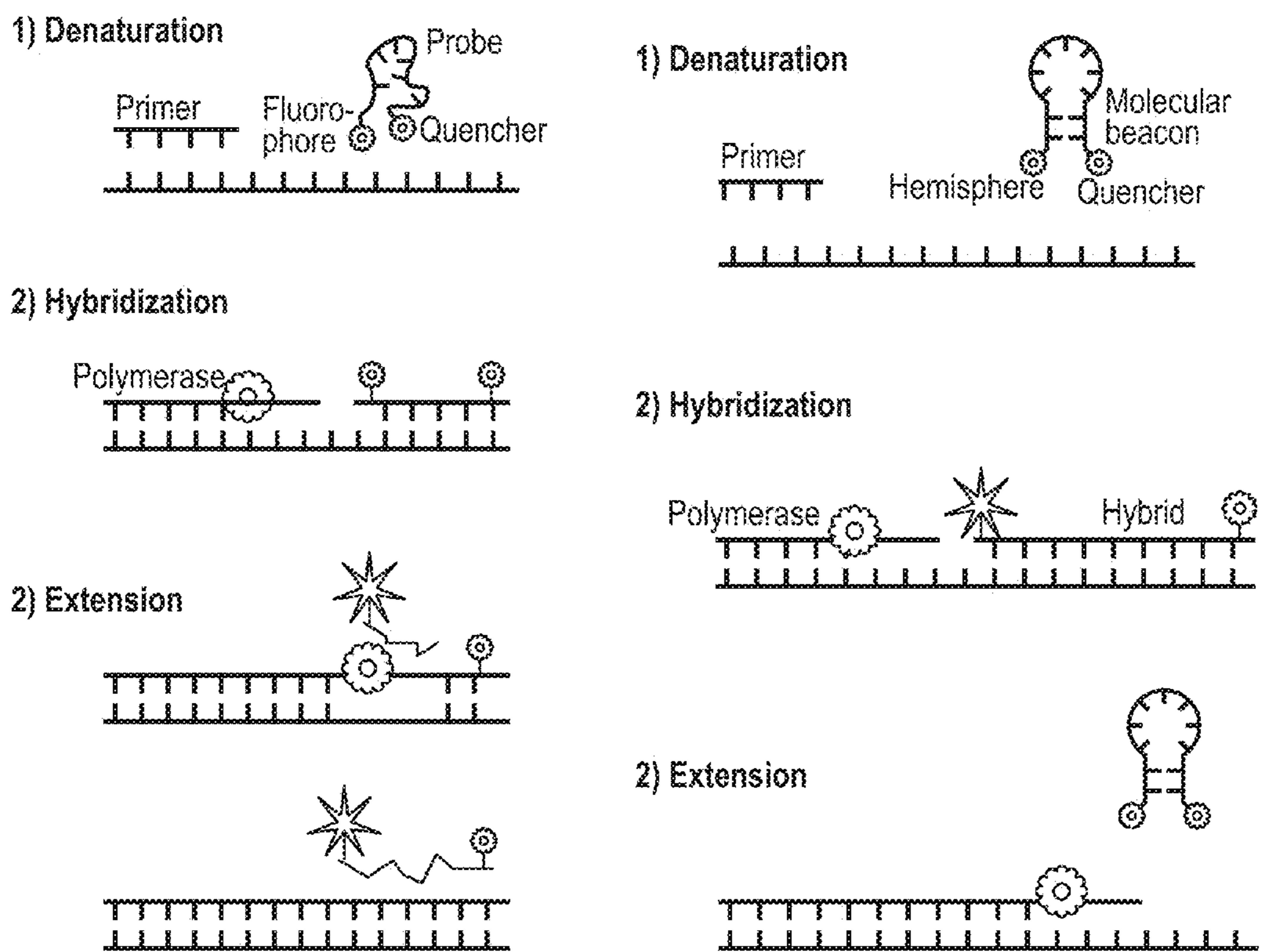
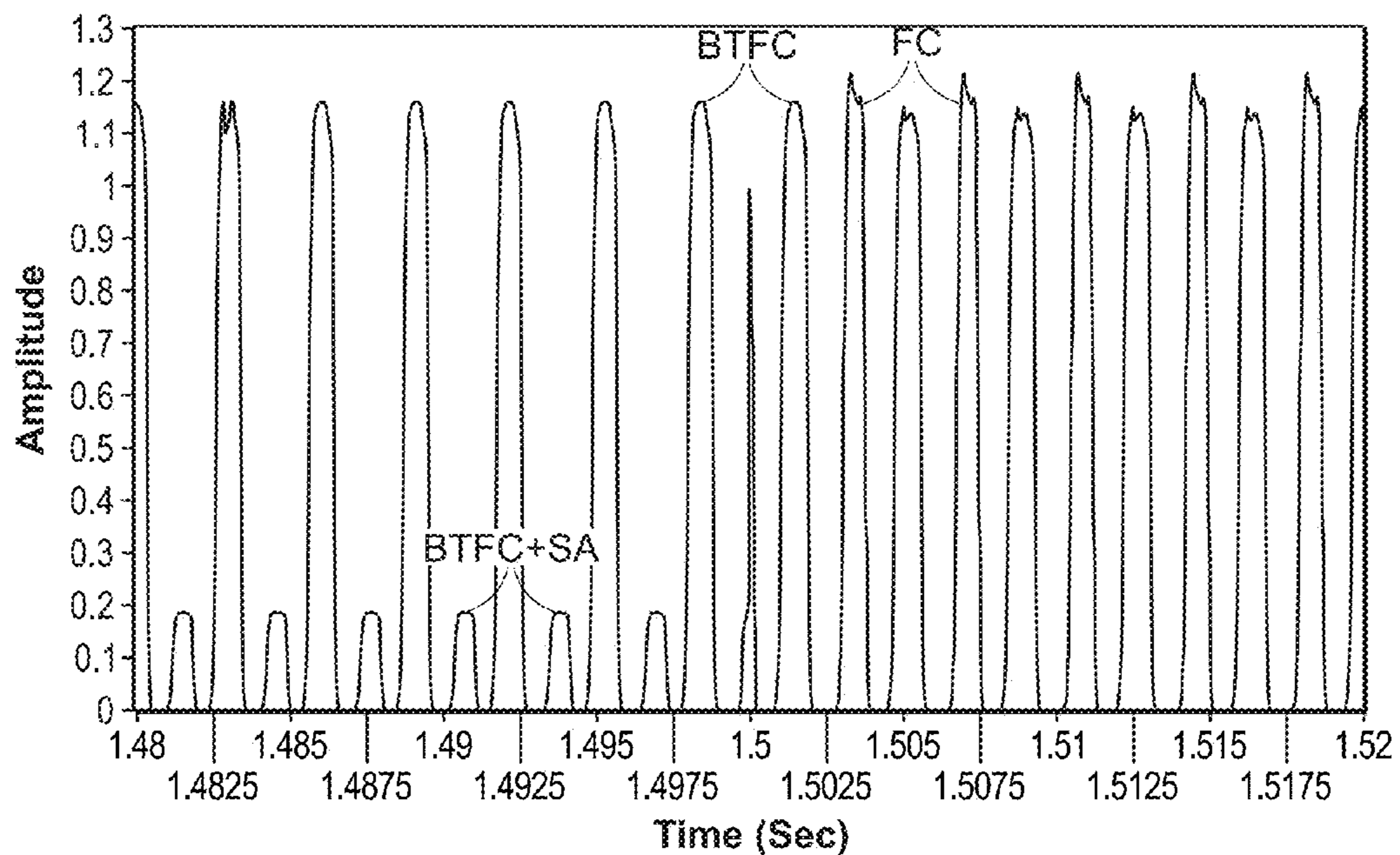


FIG. 12

Raw Data



Fluorescence Polarization

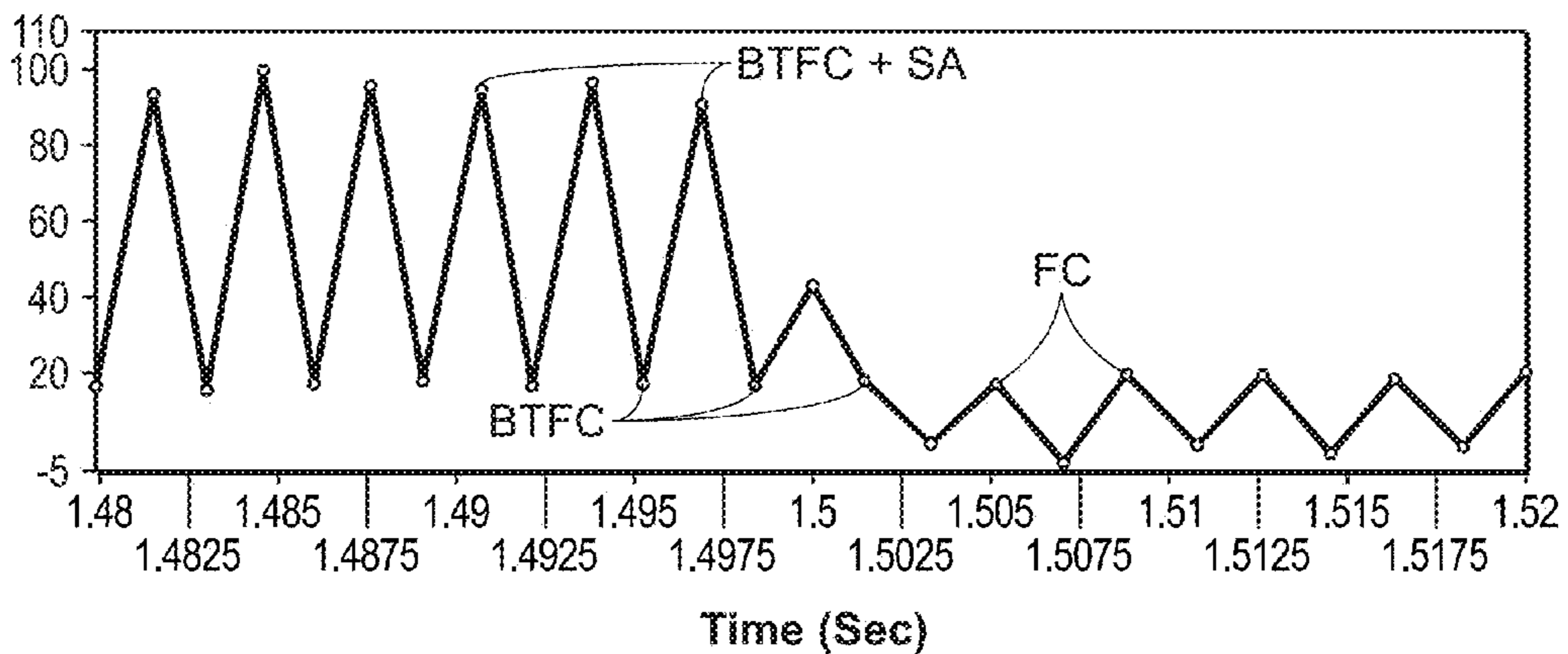


FIG. 13

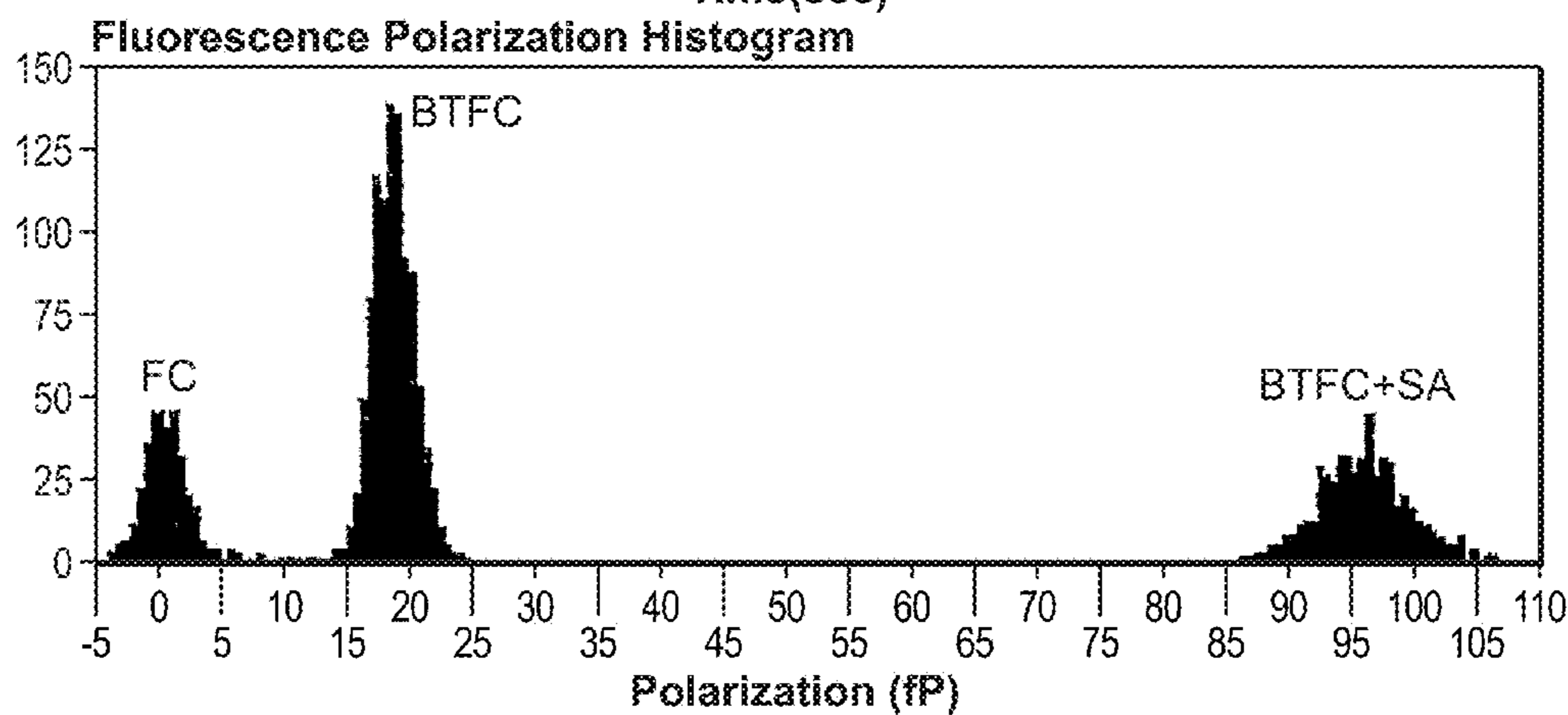
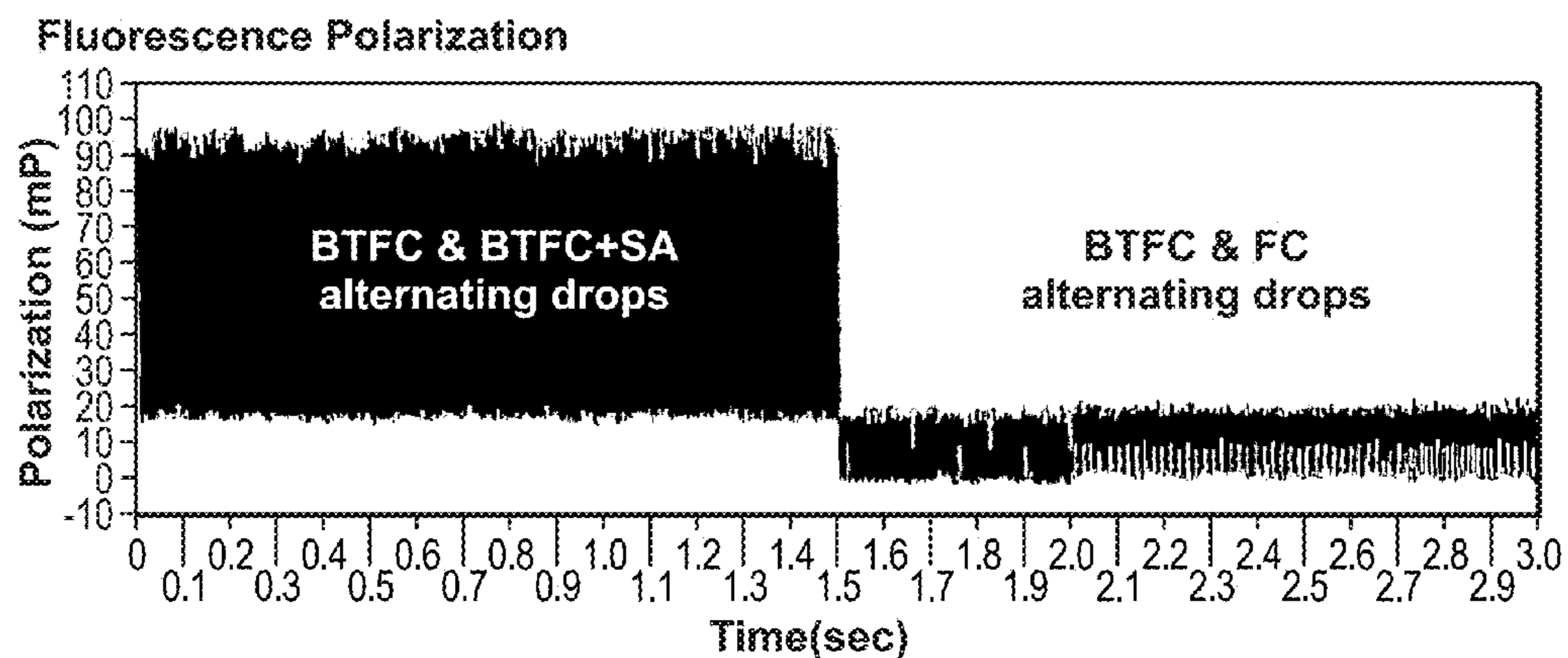


FIG. 14

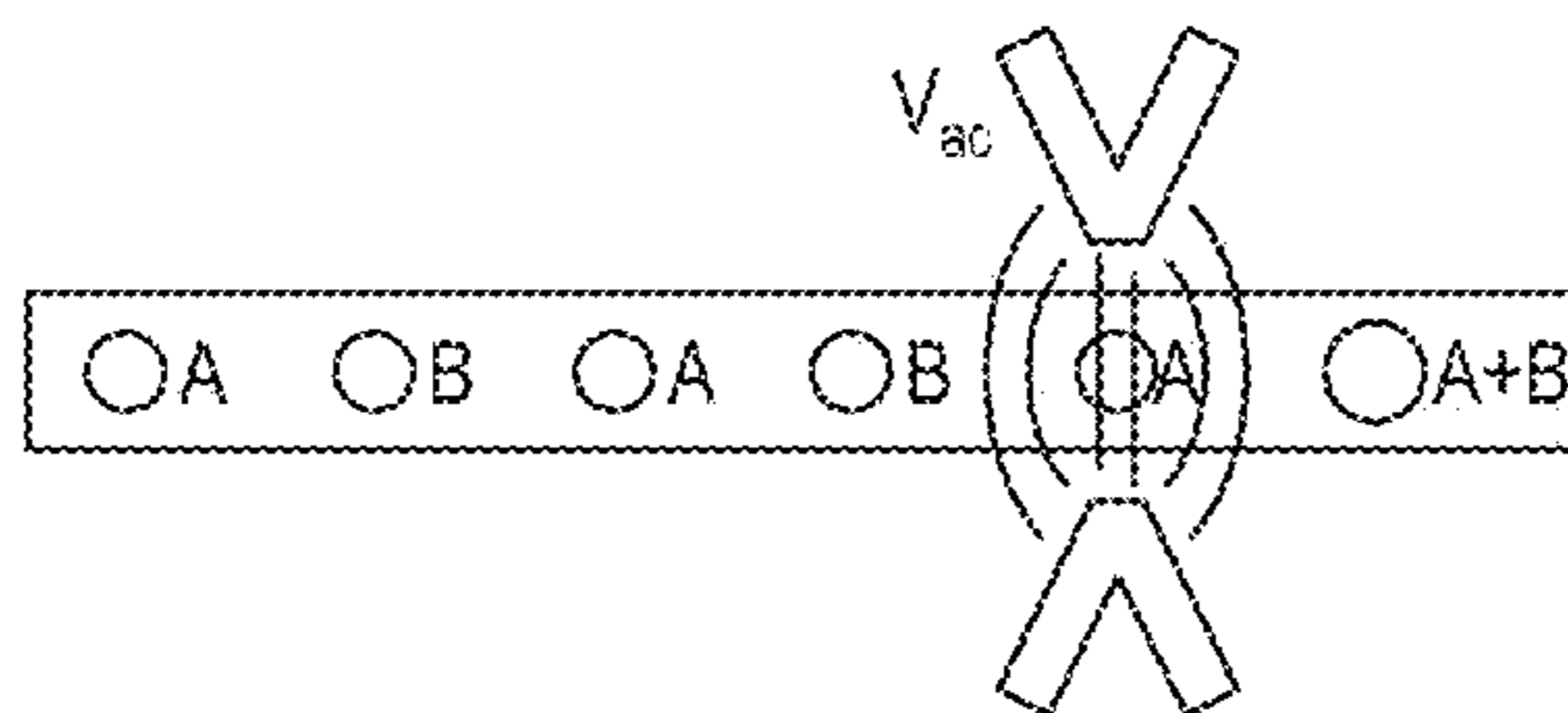


FIG. 15A

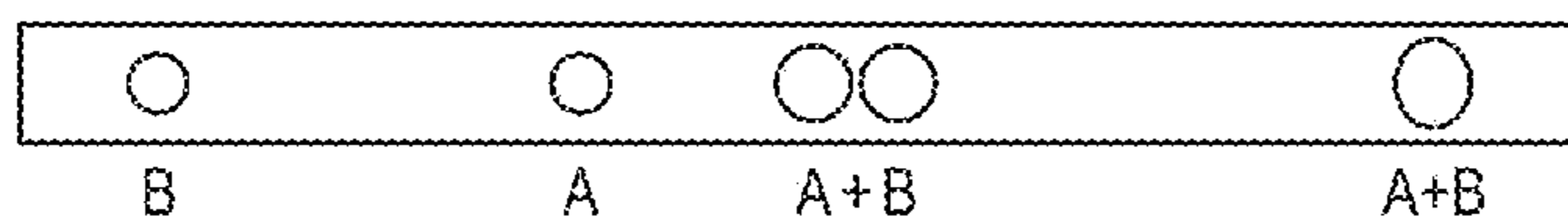


FIG. 15B

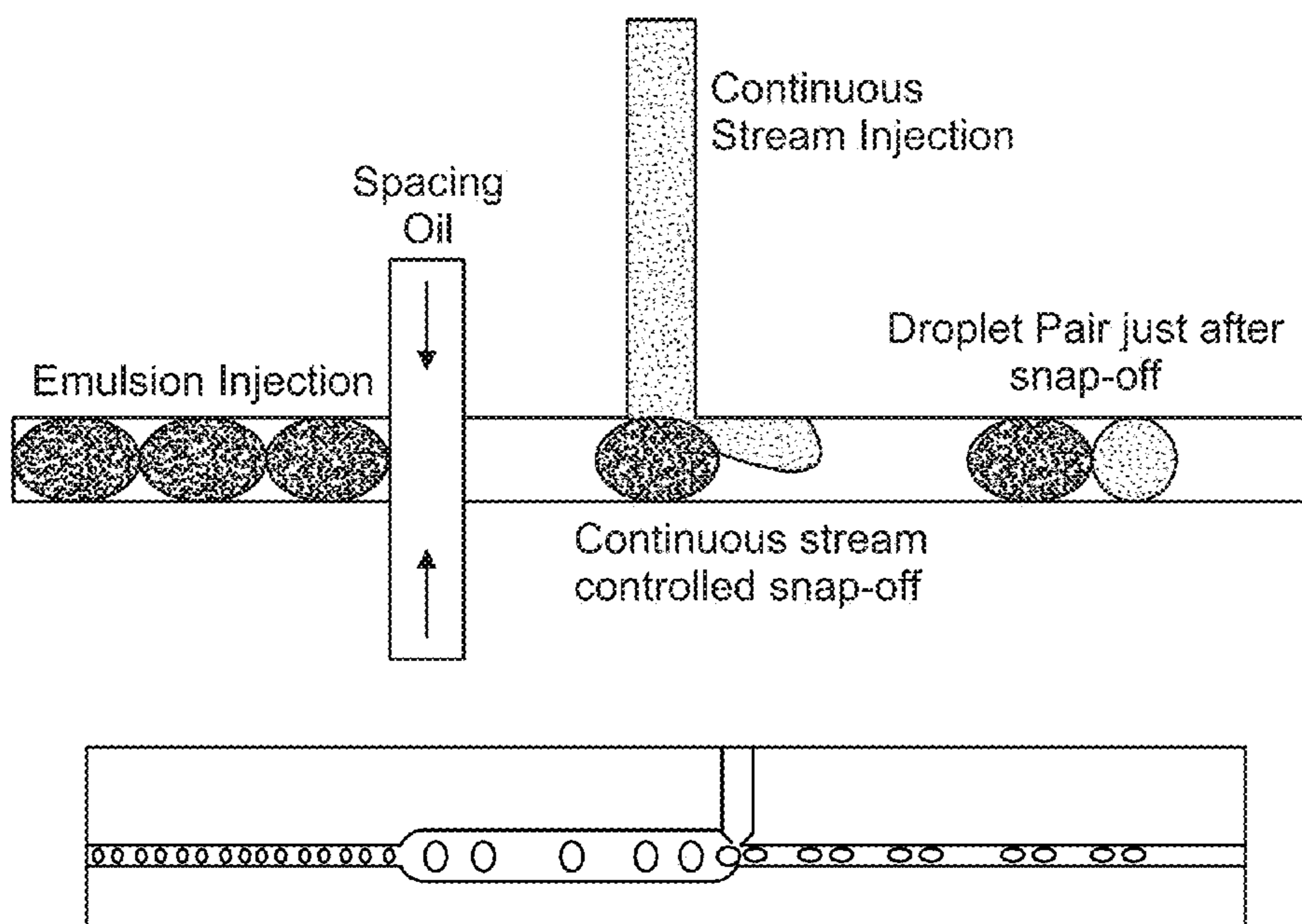


FIG. 17D



FIG. 18A

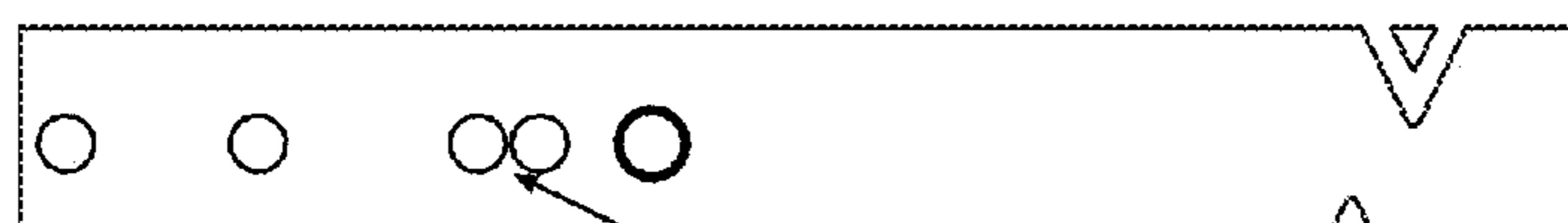


FIG. 18B

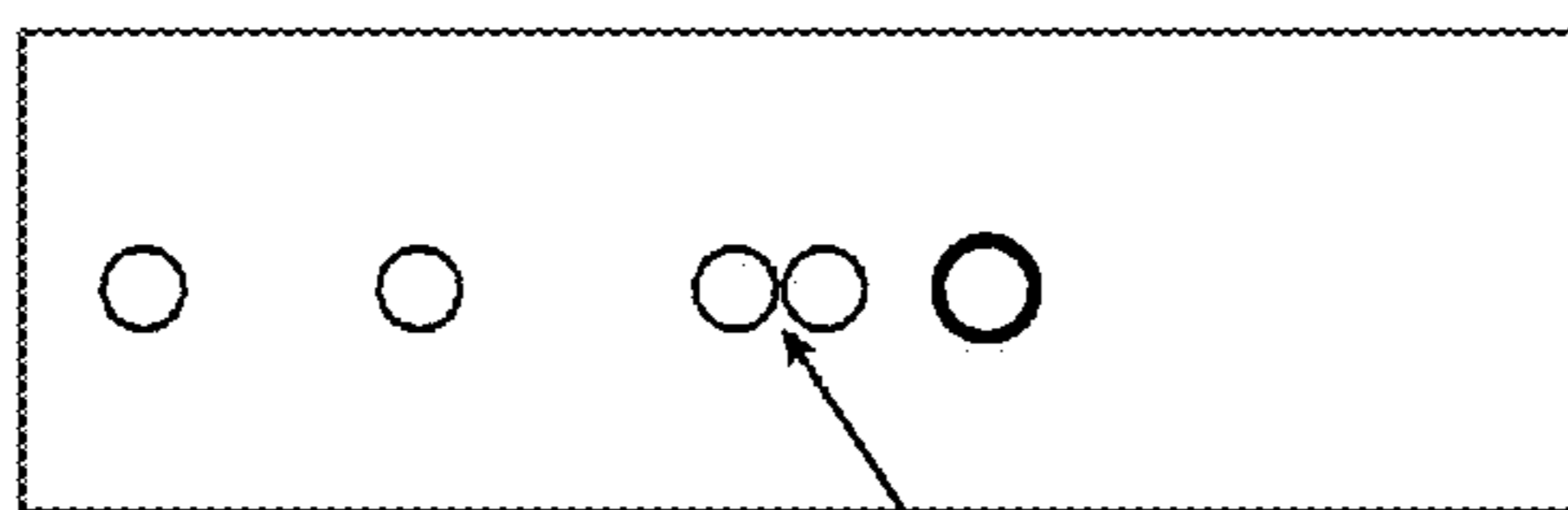


FIG. 18C



FIG. 18D

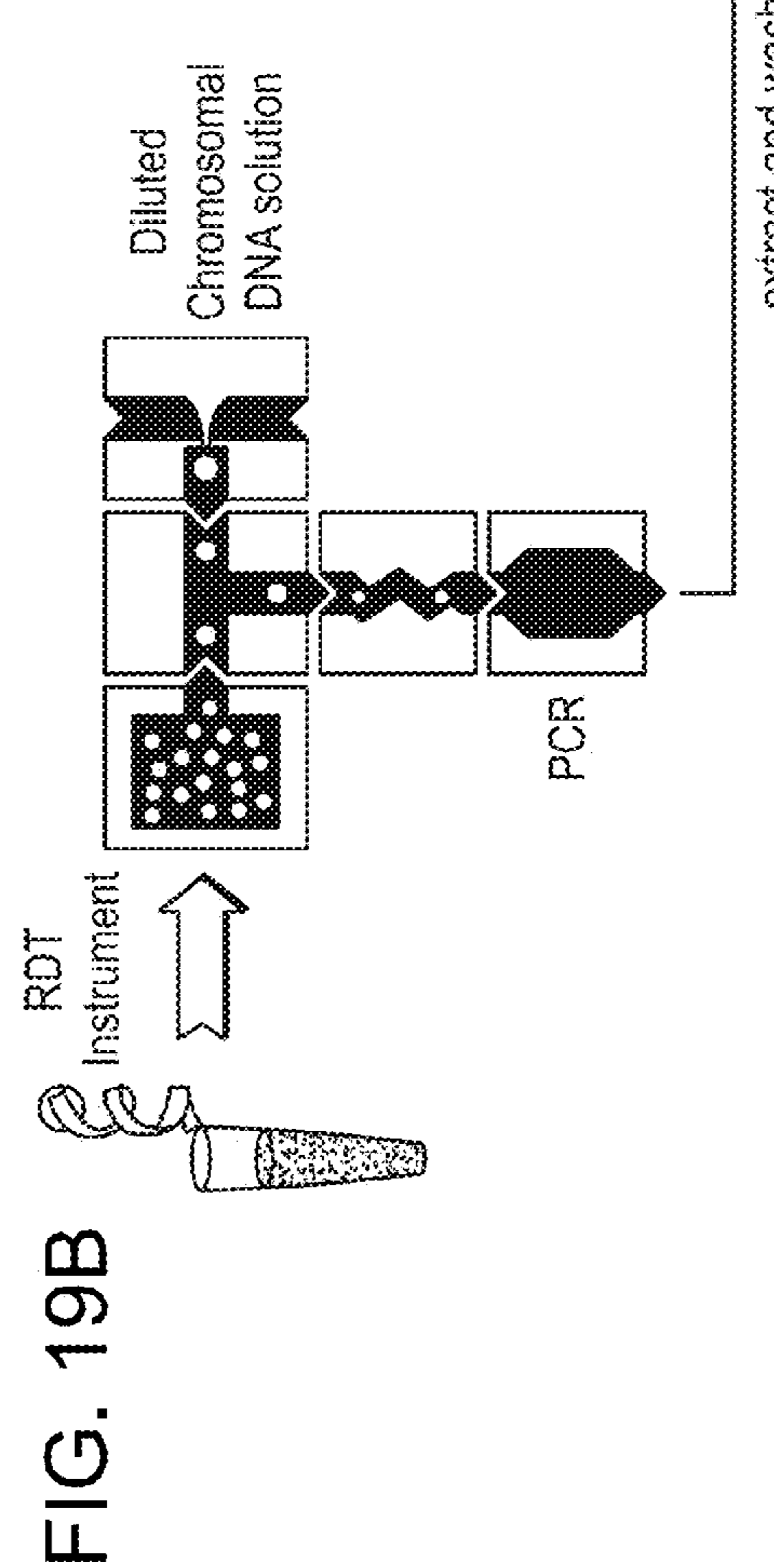
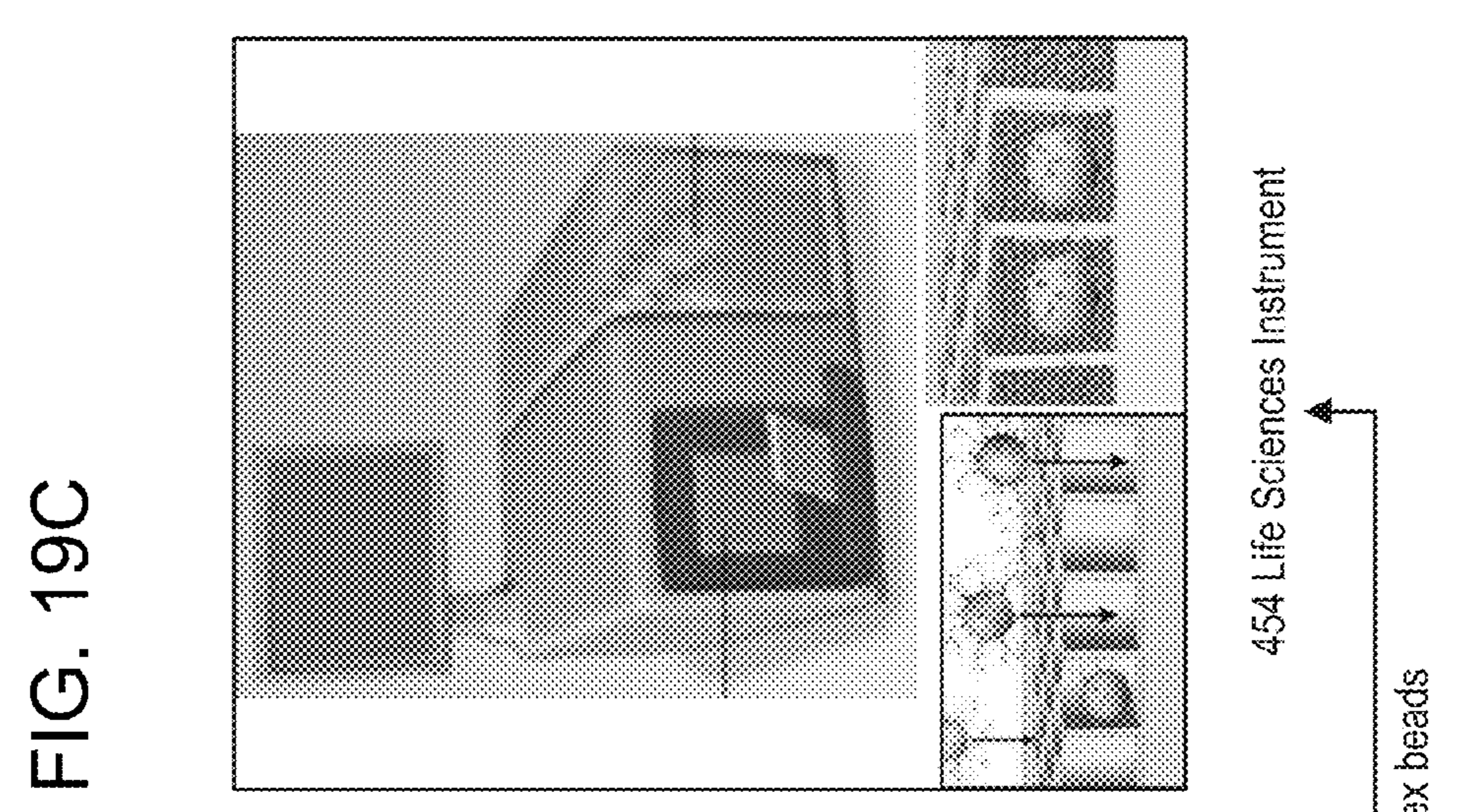
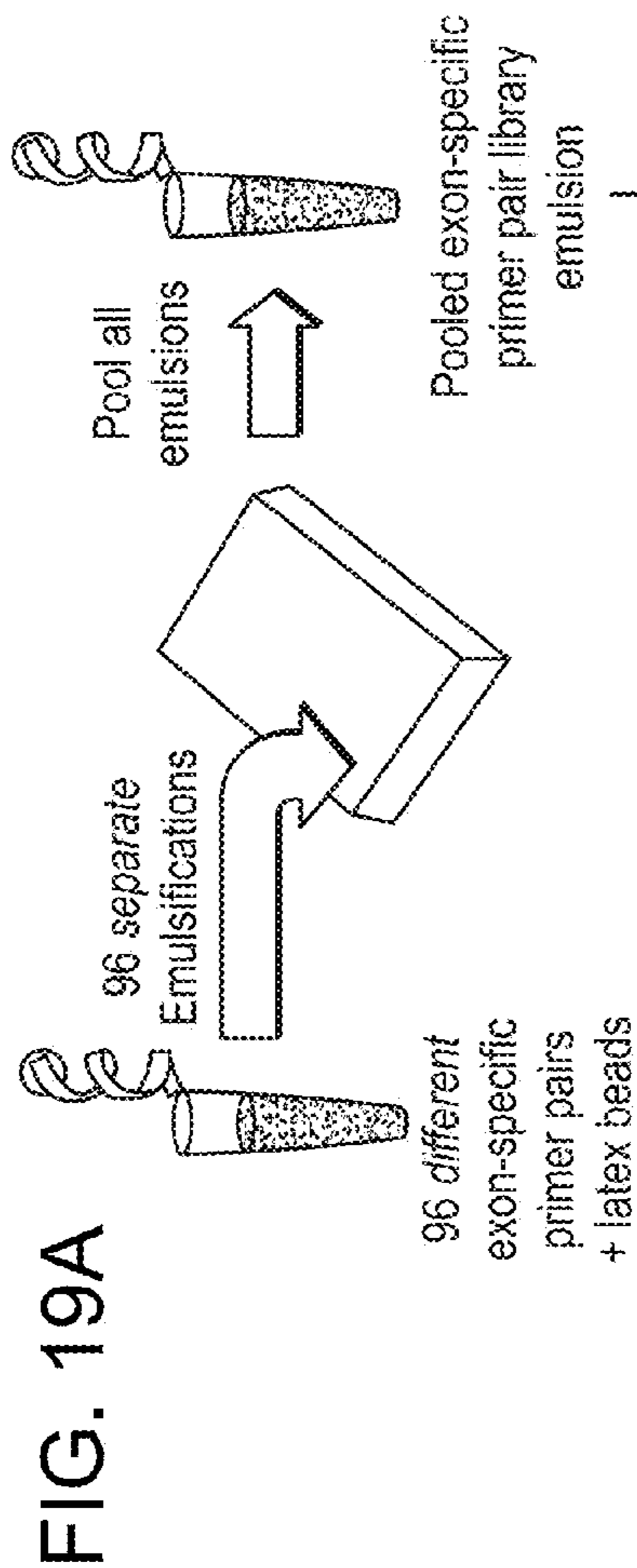


FIG. 20A

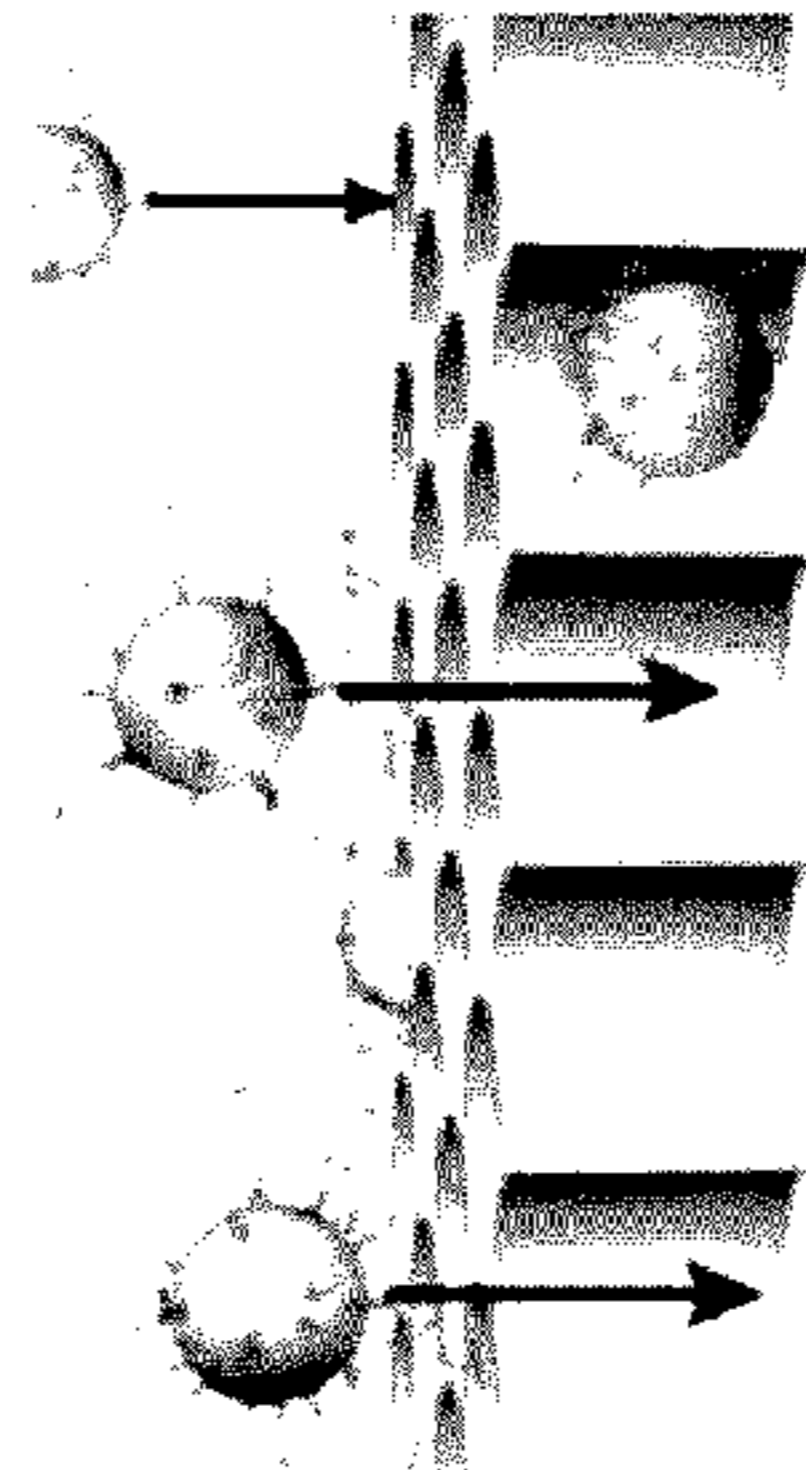
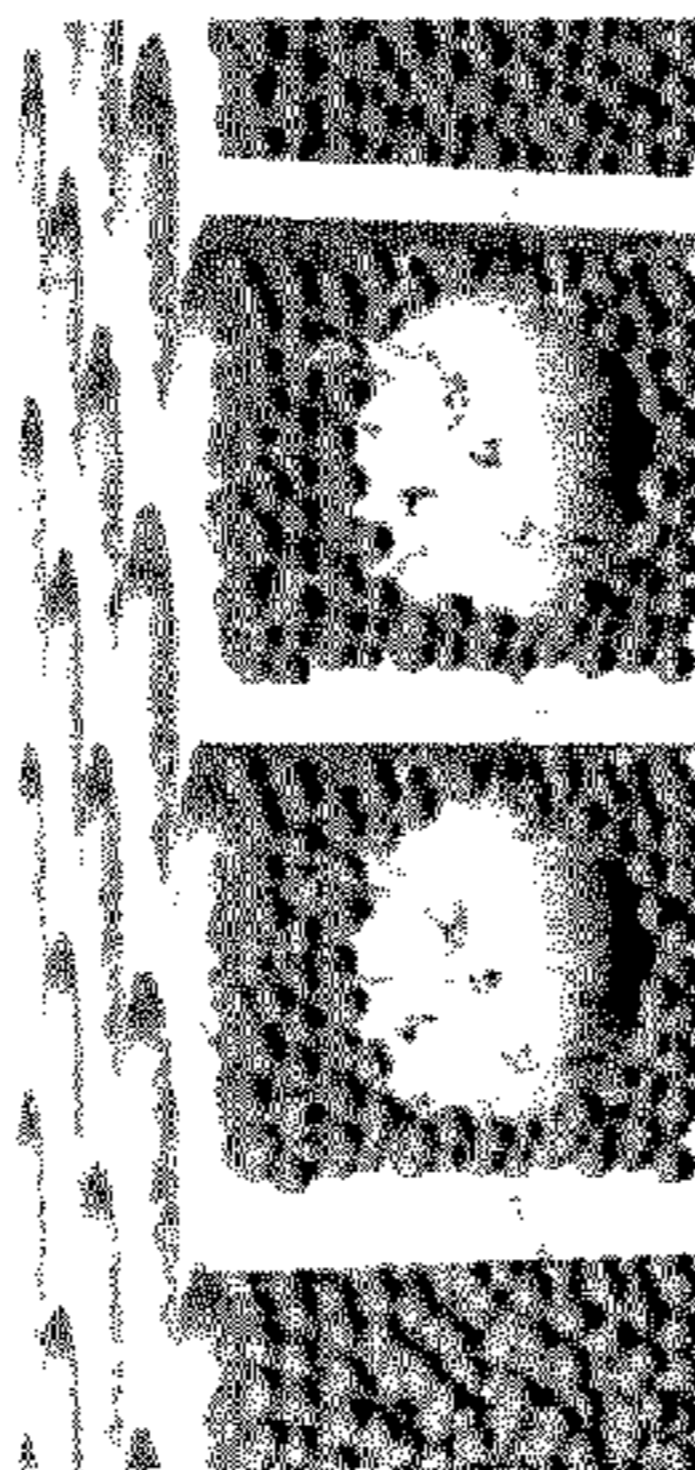
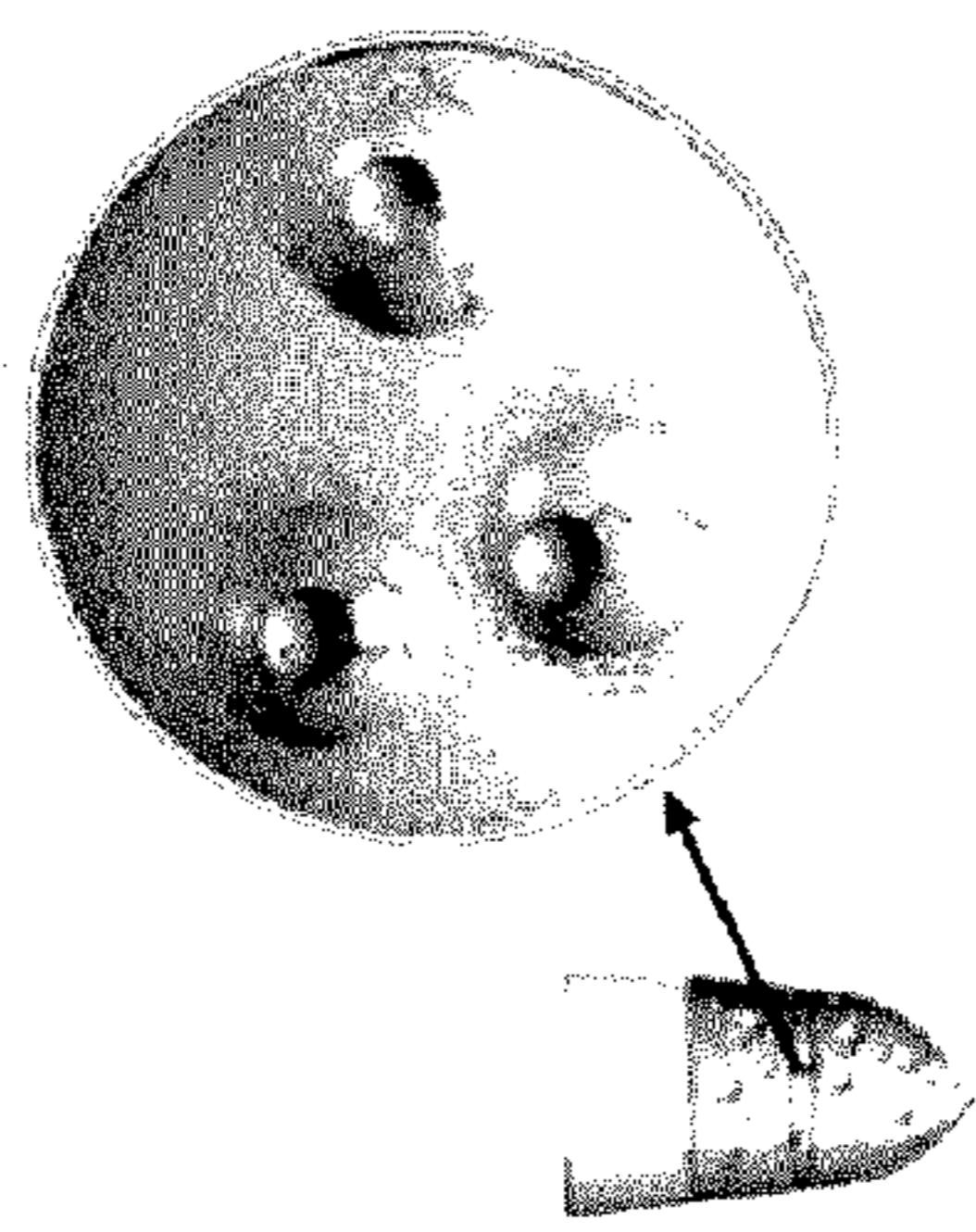
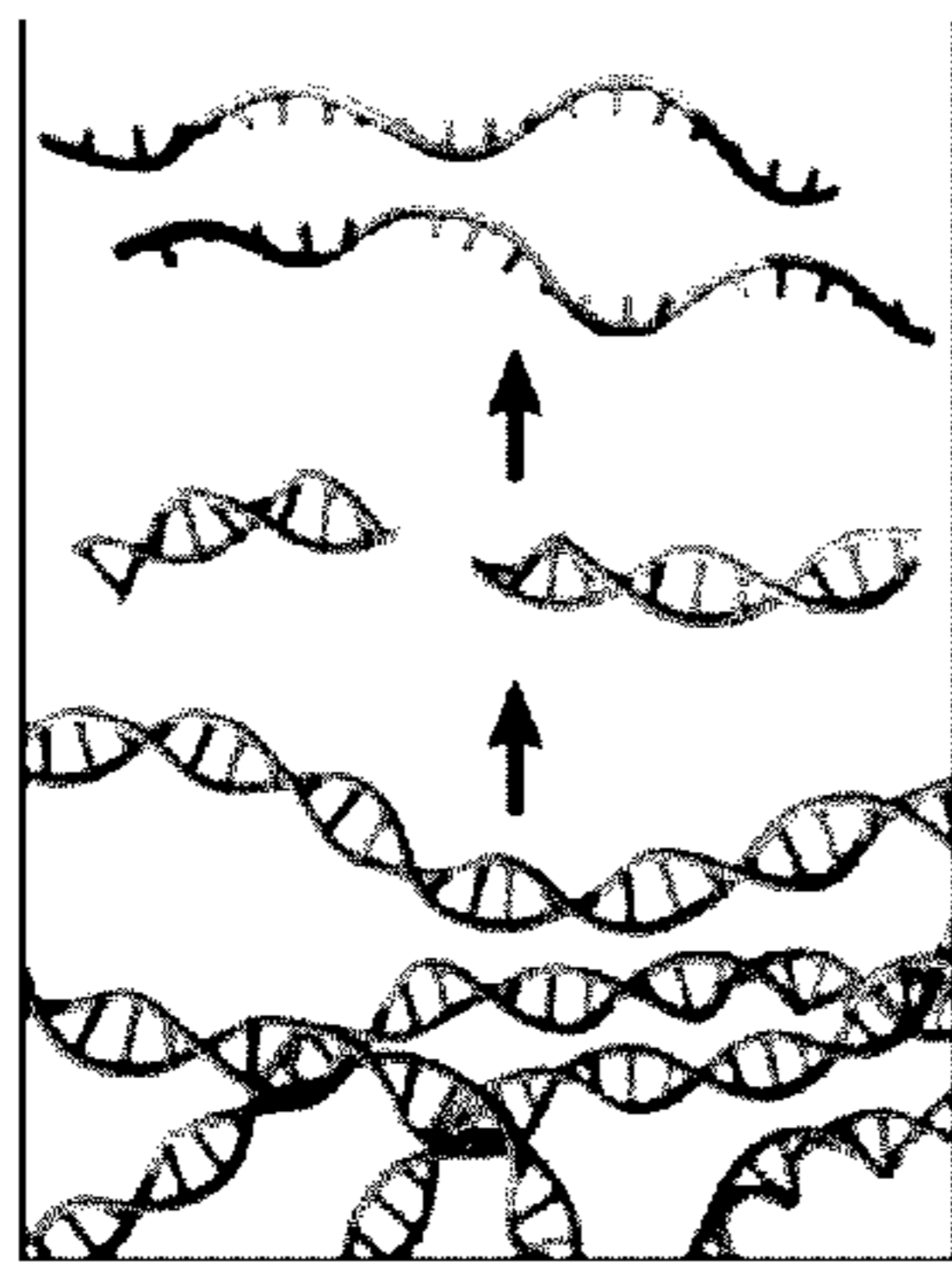


FIG. 20B

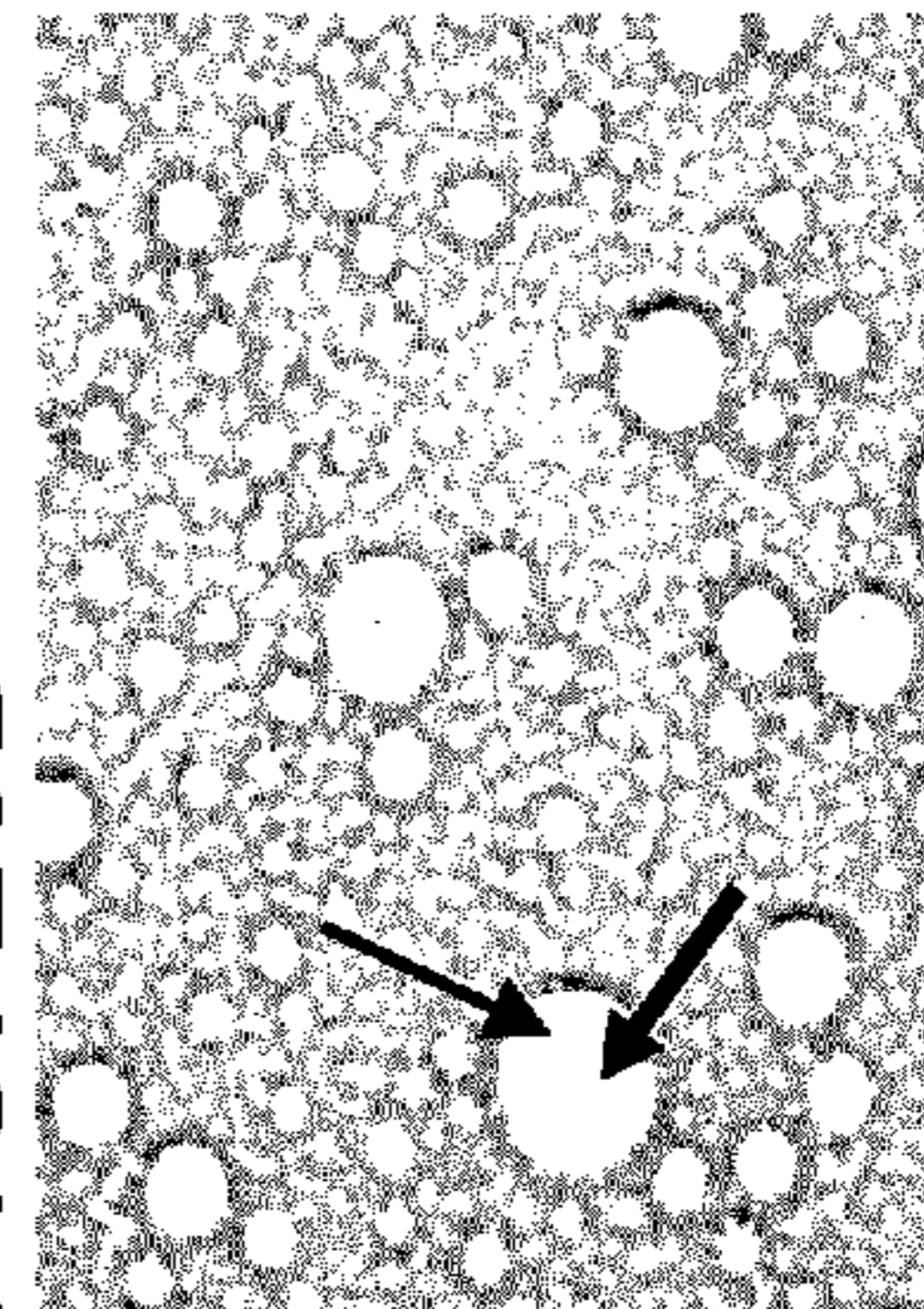


FIG. 20C

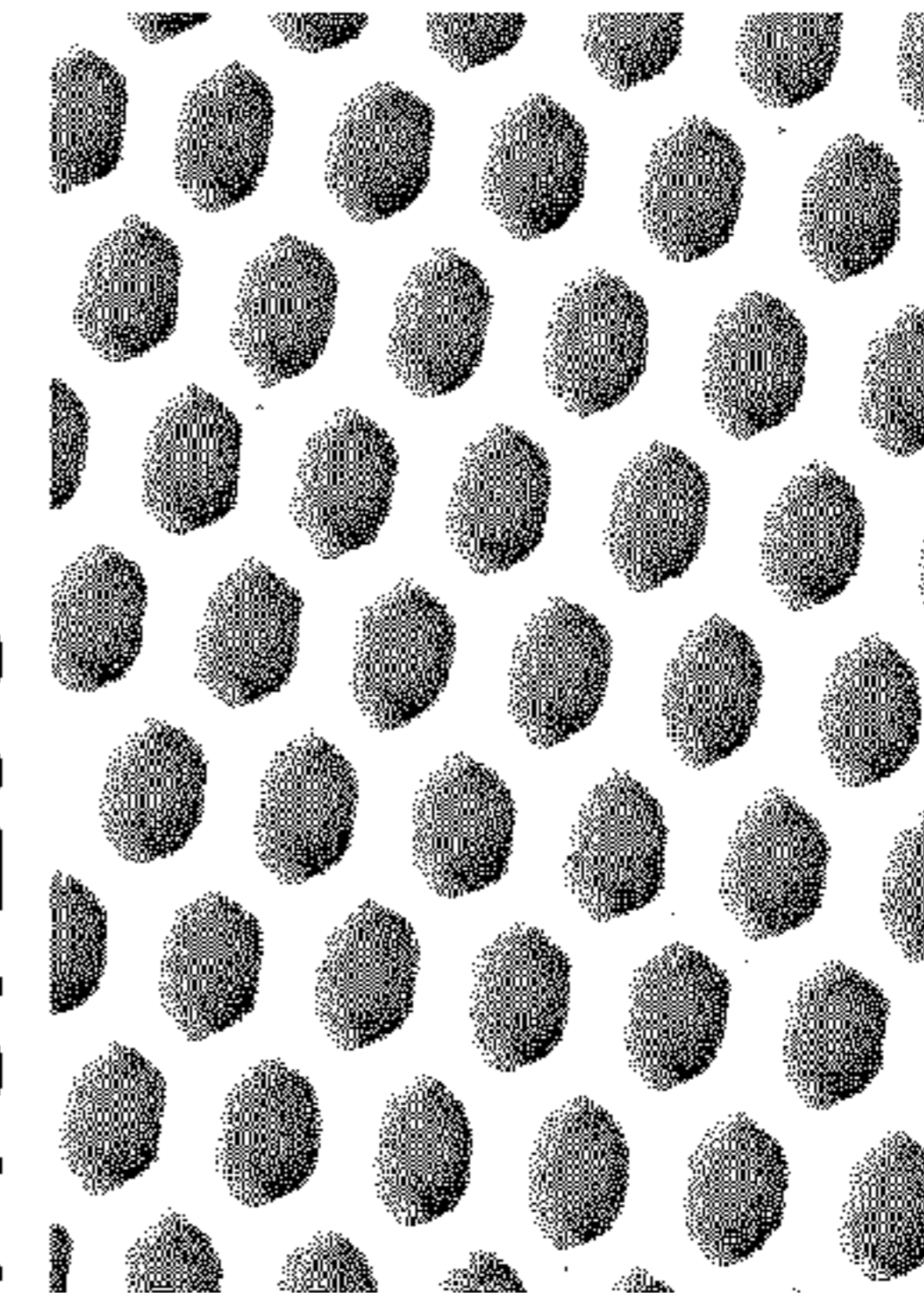
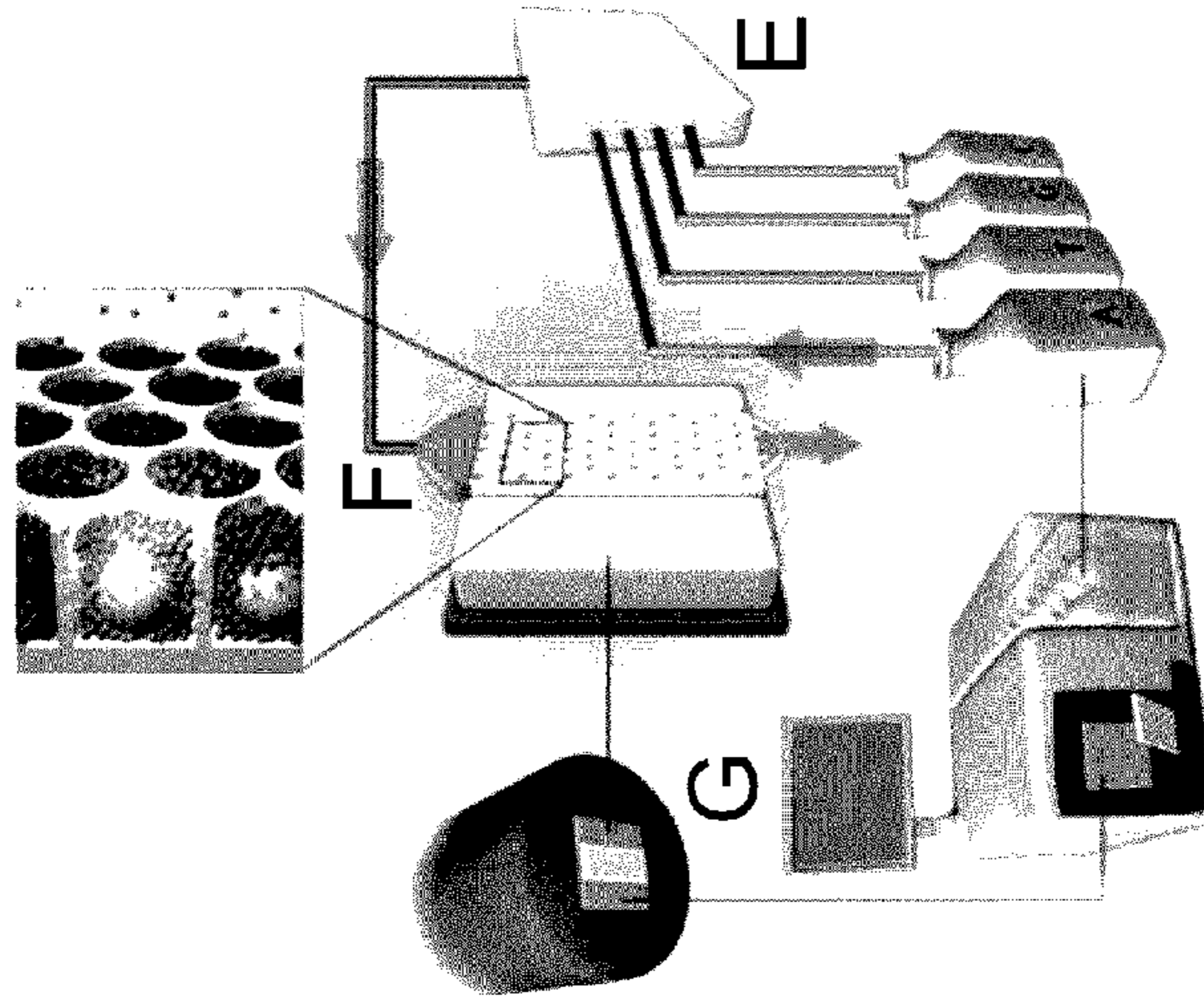


FIG. 20D



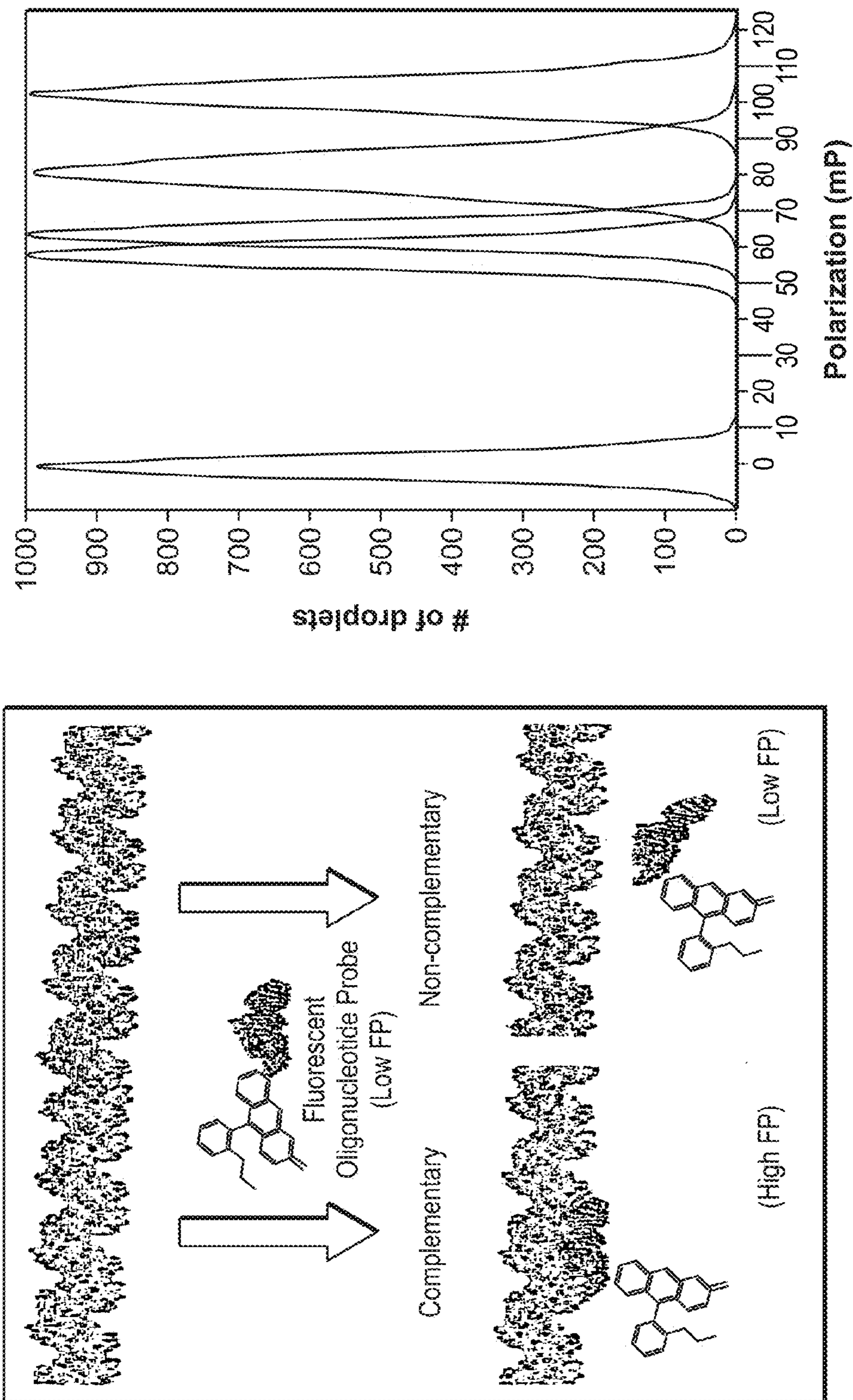


FIG. 21

**MICROFLUIDIC DEVICES AND METHODS
OF USE IN THE FORMATION AND
CONTROL OF NANOREACTORS**

RELATED APPLICATIONS

The present application is a continuation of U.S. patent application Ser. No. 13/759,660 filed Feb. 5, 2013, which is a continuation of U.S. patent application Ser. No. 12/087,713, filed Jul. 11, 2008, which is a 35 U.S.C. 371 National Phase Application of PCT/US2006/021280, filed Jun. 1, 2006, which is a Continuation-in-Part of PCT/US2006/000931, filed on Jan. 11, 2006. PCT/US2006/021280 also claims priority to, and the benefit of, U.S. Ser. No. 60/763,524 filed Jan. 30, 2006 and 60/771,286, filed Feb. 7, 2006. Each of these applications is incorporated by reference in their entirety.

FIELD OF INVENTION

The present invention generally relates to systems and methods for the formation and/or control of fluidic species, and articles produced by such systems and methods. More particularly, the present invention relates to the development of high throughput microfluidic devices for precision fluid handling and use of such systems in various biological, chemical, or diagnostic assays.

BACKGROUND

High throughput molecular screening (HTS) is the automated, rapid testing of thousands of distinct small molecules or probes in cellular models of biological mechanisms or disease, or in biochemical or pharmacological assays. Active compounds identified through HTS can provide powerful research tools to elucidate biological processes through chemical genetic approaches, or can form the basis of therapeutics or imaging agent development programs. HTS has experienced revolutionary changes in technology since the advent of molecular biology and combinatorial chemistry, and the incorporation of modern information management systems. Current HTS instrumentation allows screening of hundreds of thousands of compounds in a single day at a rate orders of magnitude greater than was possible a decade ago. However, there are still bottlenecks which currently limit HTS capacity, such as (a) compound collection maintenance, tracking, and disbursement, and (b) rapidity, accuracy, and content of assay instrumentation.

The manipulation of fluids to form fluid streams of desired configuration, discontinuous fluid streams, droplets, particles, dispersions, etc., for purposes of fluid delivery, product manufacture, analysis, and the like, is a relatively well-studied art. For example, highly monodisperse gas bubbles, less than 100 microns in diameter, have been produced using a technique referred to as capillary flow focusing. In this technique, gas is forced out of a capillary tube into a bath of liquid, where the tube is positioned above a small orifice, and the contraction flow of the external liquid through this orifice focuses the gas into a thin jet which subsequently breaks into equal-sized bubbles via a capillary instability. A similar arrangement can be used to produce liquid droplets in air.

Microfluidic systems have been described in a variety of contexts, typically in the context of miniaturized laboratory (e.g., clinical) analysis. Other uses have been described as well. For example, International Patent Application Publication No. WO 01/89788 describes multi-level microfluidic

systems that can be used to provide patterns of materials, such as biological materials and cells, on surfaces. Other publications describe microfluidic systems including valves, switches, and other components.

Precision manipulation of streams of fluids with microfluidic devices is revolutionizing many fluid-based technologies. Networks of small channels are a flexible platform for the precision manipulation of small amounts of fluids. The utility of such microfluidic devices depends critically on enabling technologies such as the microfluidic peristaltic pump, electrokinetic pumping, dielectrophoretic pump or electrowetting driven flow. The assembly of such modules into complete systems provides a convenient and robust way to construct microfluidic devices. However, virtually all microfluidic devices are based on flows of streams of fluids; this sets a limit on the smallest volume of reagent that can effectively be used because of the contaminating effects of diffusion and surface adsorption. As the dimensions of small volumes shrink, diffusion becomes the dominant mechanism for mixing leading to dispersion of reactants; moreover, surface adsorption of reactants, while small, can be highly detrimental when the concentrations are low and volumes are small. As a result, current microfluidic technologies cannot be reliably used for applications involving minute quantities of reagent; for example, bioassays on single cells or library searches involving single beads are not easily performed. An alternate approach that overcomes these limitations is the use of aqueous droplets in an immiscible carrier fluid; these provide a well defined, encapsulated microenvironment that eliminates cross contamination or changes in concentration due to diffusion or surface interactions. Droplets provide the ideal microcapsule that can isolate reactive materials, cells, or small particles for further manipulation and study. However, essentially all enabling technology for microfluidic systems developed thus far has focused on single phase fluid flow and there are few equivalent active means to manipulate droplets requiring the development of droplet handling technology. While significant advances have been made in dynamics at the macro- or microfluidic scale, improved techniques and the results of these techniques are still needed. For example, as the scale of these reactors shrinks, contamination effects due to surface adsorption and diffusion limit the smallest quantities that can be used. Confinement of reagents in droplets in an immiscible carrier fluid overcomes these limitations, but demands new fluid-handling technology.

Furthermore, the underlying physics of the influence of electric fields on fluids is well known. The attractive and repulsive forces produced by an electric field on positive or negative charges give rise to the forces on charged fluid elements, the polarization of non-polar molecules, and the torque on polar molecules which aligns them with the field. In a non-uniform field, because the force on the positively charged portion of the distribution is different than the force on the negatively charged portion, polar molecules will also experience a net force toward the region of higher field intensity. In the continuum limit, the result is a pondermotive force in the fluid. In the limit of high droplet surface tension, it is useful to describe the net pondermotive force on a droplet as if it were a rigid sphere:

$$F = qE + 2\pi R(\epsilon_m)r^3 R(K)\nabla E^2$$

where the first term is the electrophoretic force on the droplet (q is the net droplet charge and E is the electric field), and the second term is the dielectrophoretic force (r is the radius of the sphere, $R(K)$ is the real part of the Clausius-Mossotti factor

$$K = (\epsilon_p^* - \epsilon_m^*) / (\epsilon_p^* + 2\epsilon_m^*)$$

and ϵ_p^* and ϵ_m^* are the complex permittivities of the droplet and carrier fluid).

Although utility of electrophoretic control of droplets is great, it does have significant limitations. First, the charging of droplets is only effectively accomplished at the nozzle. Second, the discharge path required to eliminate screening effects also discharges the droplets. Third, finite conductivity of the carrier fluid, however small, will eventually discharge the droplets. Therefore, once the droplet is formed, there is essentially only one opportunity to perform any pondermotive function which relies on the droplet's charge density (such as coalescing oppositely charged droplets through their mutual Coulombic attraction, or electrophoretically sorting a droplet), and that function can only be performed as long as sufficient charge has not leaked off of the droplet.

Thus, it would be desirable to develop an electrically addressable emulsification system that combines compartmentalization and electrical manipulation, which allows for multi-step chemical processing, including analysis and sorting, to be initiated in confinement with exquisite timing and metering precision, for use in a variety of chemical, biological, and screening assays, in which the cost and time to perform such assays would be drastically reduced. It would also be desirable to develop a device using dielectrophoretic force (which does not rely on charge density) to manipulate droplets so that more than one electrical pondermotive function can be carried out following a significantly long delay from droplet formation.

SUMMARY OF THE INVENTION

The present invention provides devices having individual fluid handling modules that can be combined into fluid processing systems so as to perform multi-step processing of isolated components, which is essential for searching through molecular libraries for rare interactions with cells, nucleic acids, enzymes, coded microbeads, and other biomaterials. Using principles based on the electrostatic and dielectrophoretic manipulation of charged and neutral droplets 20 to 100 microns in diameter, the microfluidic devices as described herein can inexpensively encapsulate reagents, combine same, analyze, and sort in the range of 1×10^9 droplets per day. The present invention provides a microfluidic device that includes a microfabricated substrate. The substrate can include a plurality of electrically addressable channel bearing microfluidic modules integrally arranged with each other so as to be in fluid communication. The microfabricated substrate can have, for example, (i) one or more inlet modules that have at least one inlet channel adapted to carry a dispersed phase fluid, (ii) at least one main channel adapted to carry a continuous phase fluid, wherein the inlet channel is in fluid communication with the main channel such that the dispersed phase fluid is immiscible with the continuous phase fluid and forms a plurality of droplets in the continuous phase fluid, and (iii) a coalescence module downstream from and in fluid communication with the inlet modules via the main channel, wherein two or more droplets passing there through are coalesced to form a nanoreactor. The microfluidic device of the present invention can further include a sorting module, mixing module, delay module, UV-release module, detection module, collection module, waste module and/or acoustic actuator, and or combinations thereof, in any order. These modules are in

fluid communication with the main channel. The flow of the dispersed phase and continuous phase can be pressure driven, for example.

The present invention also provides methods of creating a nanoreactor. The method includes, for example, a) providing a microfabricated substrate having a plurality of electrically addressable channel bearing microfluidic modules integrally arranged on the substrate so as to be in fluid communication with each other, thereby forming at least one main channel adapted to carry at least one continuous phase fluid; b) flowing a first dispersed phase fluid through a first inlet channel into the main channel such that one or more droplets is formed in the continuous phase fluid flowing therein; c) flowing a second dispersed phase fluid through a second inlet channel into the main channel such that one or more droplets is formed in the continuous phase fluid flowing therein; and d) coalescing at least one droplet formed in step (b) with at least one droplet formed in step (c) as the droplets pass through a coalescence module of the microfabricated substrate, thereby producing a nanoreactor. The coalescing step can be achieved by an electric field or passively. The first and second dispersed phase fluids can include a biological or chemical material, which can include, for example, tissues, cells, particles, proteins, antibodies, amino acids, nucleotides, small molecules, and pharmaceuticals. The nanoreactor can further be incubated within a delay module, and then interrogated for a predetermined characteristic within a detection module.

The present invention also includes methods of synthesizing a compound from two or more reactive substructures. In a particular aspect the method includes a) labeling the reactive substructures with a label unique to the substructure; b) emulsifying aqueous solutions of the labeled reactive substructures on a microfluidic device to form droplets; and c) randomly combining the droplets on the microfluidic device to form a compound. The one embodiment, the method further includes d) screening the compound formed in step (c) based on a desirable chemical or biological property exhibited by the compound; and e) identifying the structure of the compound by decoding the label. In another embodiment, steps (a) and (b) are alternatively performed by introducing a preformed labeled emulsion.

In another aspect, the present invention provides methods for identifying a single compound from a library on a microfluidic device. The method can include a) labeling a library of compounds by emulsifying aqueous solutions of the compounds and aqueous solutions of unique liquid labels, whereby each compound is labeled with a unique liquid label; b) pooling the labeled emulsions resulting from step (a); c) coalescing the labeled emulsions with emulsions containing a specific cell or enzyme, thereby forming a nanoreactor; d) screening the nanoreactors for a desirable reaction between the contents of the nanoreactor; and e) decoding the liquid label, thereby identifying a single compound from a library of compounds. In various embodiments of the method, the contents of the nanoreactor can be incubated prior to screening. The screening step can be performed by fluorescent polarization, for example. The liquid label can be a quantum dot (q-dot) or a dye.

In yet another aspect, the present invention includes methods for controlling the quality of a library of emulsified compounds. The method can include, for example, a) providing a library of emulsified compounds; b) emulsifying a q-dot encoded aqueous buffer in an inert fluorocarbon medium, thereby forming droplets; c) incubating the q-dot encoded droplet with the library of emulsified compounds; d) sorting the q-dot encoded droplet away from the library;

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e) analyzing the q-dot encoded droplet for the presence of any of the compounds emulsified in the library; and f) eliminating the compounds identified in step (e) from the library of emulsified compounds, wherein one or more of steps (a)-(f) are performed on a microfluidic device. In one embodiment, the analyzing step is performed by mass spectroscopy.

In still a further aspect, the present invention provides methods for sorting cells. The method can include a) fusing an affinity-reagent to an enzyme; b) mixing the fusion product of step (a) with a cell population; c) isolating cells attached to the fusion product; d) emulsifying the cells of step (c) in an inert fluorocarbon medium; e) coalescing the cell emulsion of step (d) with an emulsion comprising a substrate corresponding to the enzyme of step (a), thereby forming a nanoreactor; and f) screening the nanoreactor for a desirable reaction between the contents of the nanoreactor, wherein one or more steps of (a)-(f) are performed on a microfluidic device. In one embodiment, the affinity-reagent can be an antibody that is specific for a cell-surface cancer marker. The enzyme can include alk/phos, β -galactosidase, or horseradish peroxidase. The affinity-reagent can be fused to multiple enzymes, and multiple substrates can be emulsified and coalesced with the cell emulsions.

Another aspect of the present invention provides methods for sequencing individual exons from individual chromosomes. The method can include, for example, a) emulsifying specific primer-pairs to an exon with beads that can bind to said primer-pairs; b) pooling the emulsions of step (a) to create a library emulsion; c) providing a separate chromosomal DNA emulsion; d) coalescing the library emulsion of step (b) with the chromosomal emulsion of step (c), thereby forming a nanoreactor; e) amplifying the DNA in the nanoreactor; f) isolating the beads; g) screening for beads containing DNA; and h) sequencing the beads containing DNA, wherein one or more steps of (a)-(h) are performed on a microfluidic device.

BRIEF DESCRIPTION OF DRAWINGS

Non-limiting embodiments of the present invention will be described by way of example with reference to the accompanying drawings, which are schematic and are not intended to be drawn to scale. In the drawings, each identical or nearly identical component illustrated is typically represented by a single numeral. For the purposes of clarity, not every component is labeled in every drawing, nor is every component of each embodiment of the invention shown where illustration is not necessary to allow those of ordinary skill in the art to understand the invention. In the drawings:

FIG. 1 is a schematic illustrating the interacting modules of a microfluidic device of the present invention.

FIG. 2 is a photograph and accompanying graphs showing the flow cytometric-cell-based assay for human and bacterial cells.

FIG. 3 is a schematic and graph showing simultaneous two color fluorescence detection.

FIG. 4 is a schematic illustrating chemical library screening using a nanoreactor of the present invention.

FIG. 5 is a schematic illustrating the physical basis of fluorescence polarization assays.

FIG. 6 is several graphs showing the absorption and emission spectra of q-dots and organic dye.

FIG. 7 is a schematic showing the extension to the fluorescence test station required to perform polarization fluorescence measurements simultaneously with q-dot read-out.

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FIG. 8 is a schematic and accompany graphs showing a fluorescence polarization based kinase assay.

FIG. 9 is a schematic illustrating the retrosynthetic analysis of Gleevec.

FIG. 10 is a schematic illustrating the synthesis of a fluorescent and non-fluorescent product from the same precursor.

FIG. 11 is schematic showing the use of nucleic acids for chemical encoding and decoding tagging of chemical reactions.

FIG. 12 is a schematic illustrating a taqman assay and molecular beacon probes.

FIG. 13 is a graph showing polarized fluorescence signals.

FIG. 14 is a graph showing a time trace and histogram of fluorescence polarization calculated from analyzed droplets.

FIG. 15 (A) is a schematic illustrating dielectrophoretic stopping of droplet A allowing droplet B to contact A and coalesce. The dielectrophoretic force is not strong enough to stop the combined A+B and they move off in the stream. This is shown in the photomicrograph, FIG. 15 (B).

FIG. 16 is a schematic (a) and photographs (b, e) showing droplets made on-chip (A) being interdigitated with library droplets (B). The droplets are of different size and the smaller droplets B move at a higher velocity than droplets A until they catch up after which they move together. An electric field causes the droplets to coalesce, FIG. 16 (c). Droplets A and B may both come from libraries (made off-chip) FIG. 16 (d), or be made on-chip.

FIG. 17 (A-D) shows alternate ways to achieve interdigitiation of droplets of different type.

FIG. 18A-D highlight observed passive coalescence of coupled droplet pairs—(A) Tee 0.25 mM FC-1% E5-5% PVP 70-FF1% E5-5% PVP-0.1 mM FC-PBS 70-11172005-nozzles-3.cin; (B) Tee 0.25 mM FC-1% E5-5% PVP 90-FF 1% E5-5% PVP-0.1 mM FC-PBS 70-11172005-nozzles-5.cin; (C) Tee 0.25 mM FC-1% E5-5% PVP 90-FF 1% E5-5% PVP-0.1 mM FC-PBS 70-11172005-nozzles-prior to coalesce-8.cin; (D) 1% E5-5% PVP-0.25 mM FC-50-1% E5-5% PVP-O. 1 mM FC-PBS 50-11172005-overview-1.cin.

FIG. 19 shows a schematic diagram of the assembly of modules used for sequencing exons of individual chromosomes. (A) Individual specific primer-pairs to different exons along with a primer-bound bead are each separately emulsified and then pooled to create a library emulsion (a set of 96 exon primer pairs are shown for illustrative purposes); (B) Individual modules are strung together in a sequence of droplet operations. A chromosomal DNA solution is diluted such that a 30 micron drop contains, on average, slightly less than a half-genome's concentration of DNA. Droplets from the pooled emulsion library set of exon-specific primers are combined with droplets containing the diluted solution of chromosomal DNA and used in a bead-based DNA amplification reaction (i.e., PCR); (C) The DNA-containing beads will be randomly placed into a picotiter plate and sequenced using a 454 Corp.'s Life Sciences DNA sequencing instrument.

FIG. 20 describes sample preparation and DNA sequencing on the 454 Instrument. A) Genomic DNA is isolated, fragmented, ligated to adapters and separated into single strands (top left). Fragments are bound to beads under conditions that favor one fragment per bead, the beads are captured in the droplets of a PCR-reaction-mixture-in-oil emulsion and PCR amplification occurs within each droplet, resulting in beads each carrying ten million copies of a unique DNA template (top, second from the left). The emulsion is broken, the DNA strands are denatured, and

beads carrying single-stranded DNA clones are deposited into wells of a fiber-optic slide (bottom left). Smaller beads carrying immobilized enzymes required for pyrophosphate sequencing are deposited into each well (bottom, second from the left); B) Microscope photograph of emulsion showing droplets containing a bead and empty droplets. The thin arrow points to a 28- μ m bead; the thick arrow points to an approximately 100- μ m droplet; C) Scanning electron micrograph of a portion of a fiber-optic slide, showing fiber-optic cladding and wells before bead deposition; D) The sequencing instrument consists of the following major subsystems: a fluidic assembly; E) a flow chamber that includes the well-containing fiber-optic slide; F) a CCD camera-based imaging assembly; G) and a computer that provides the necessary user interface and instrument control.

FIG. 21 shows measurement of DNA hybridization using fluorescence polarization (FP) on the microfluidic device described herein. (A) FP can be used to measure the binding of 2 DNA molecules on the microfluidic device. (B) Oligonucleotide 102 is complement to both 101 and 103. The addition of either oligonucleotide to the labeled 102 shifts the mP value, indicative of binding. Addition of 102 to non-complementing oligos does not change its mP (data not shown). Oligonucleotides; #101: 5' Biotin—ATCCGC-CCCAGCA GCTGCCAGGCACAGCCCCTAACTCCTGATTTATGCTGCATCCATTTTGC 3'(SEQ ID NO: 1); #102: 5' Fluorescein—GCAAATGGATGCAG-CATAAATCAGGAGTTTAG 3'(SEQ ID NO: 2); #103: 5' Fluorescein—CTAACTCCTGATTTA TGCTGCATC-CATTTTGC-3'(SEQ ID NO: 3).

DETAILED DESCRIPTION

The microfluidic devices and methods of use described herein are based on the creation and electrical manipulation of aqueous phase droplets completely encapsulated by an inert fluorocarbon oil stream. This combination enables electrically addressable droplet generation, highly efficient droplet coalescence, precision droplet breaking and recharging, and controllable single droplet sorting. Additional passive modules include multi-stream droplet formulations, mixing modules, and precision break-up modules. The integration of these modules is an essential enabling technology for a droplet based, high-throughput microfluidic reactor system. The microfluidic devices of the present invention can use a flow-focusing geometry to form the droplets. For example, a water stream can be infused from one channel through a narrow constriction; counter propagating oil streams (preferably fluorinated oil) hydrodynamically focus the water stream and stabilize its breakup into micron size droplets as it passes through the constriction. In order to form droplets, the viscous forces applied by the oil to the water stream must overcome the water surface tension. The generation rate, spacing and size of the water droplets is controlled by the relative flow rates of the oil and the water streams and nozzle geometry. While this emulsification technology is extremely robust, droplet size and rate are tightly coupled to the fluid flow rates and channel dimensions. Moreover, the timing and phase of the droplet production cannot be controlled. To overcome these limitations, the microfluidic devices of the present invention can incorporate integrated electric fields, thereby creating an electrically addressable emulsification system. In one embodiment, this can be achieved by applying high voltage to the aqueous stream and charge the oil water interface. The water stream behaves as a conductor while the oil is an insulator; electrochemical reactions charge the fluid interface like a

capacitor. At snap-off, charge on the interface remains on the droplet. The droplet size decreases with increasing field strength. At low applied voltages the electric field has a negligible effect, and droplet formation is driven exclusively by the competition between surface tension and viscous flow, as described above. The microfluidic, droplet-based reaction-confinement system of the present invention can further include a mixer which combines two or more reagents to initiate a chemical reaction. Multi-component droplets can easily be generated by bringing together streams of materials at the point where droplets are made. However, all but the simplest reactions require multiple steps where new reagents are added during each step. In droplet-based microfluidic devices, this can be best accomplished by combining {i.e. coalescing} different droplets, each containing individual reactants. However, this is particularly difficult to achieve in a microfluidic device because surface tension, surfactant stabilization, and drainage forces all hinder droplet coalescence; moreover, the droplets must cross the stream lines that define their respective flows and must be perfectly synchronized to arrive at a precise location for coalescence. The microfluidic devices of the present invention overcome these difficulties by making use of electrostatic charge, placing charges of opposite sign on each droplet, and applying an electric field to force them to coalesce. By way of non-limiting example, a device according to the present invention can include two separate nozzles that generate droplets with different compositions and opposite charges. The droplets are brought together at the confluence of the two streams. The electrodes used to charge the droplets upon formation also provide the electric field to force the droplets across the stream lines, leading to coalescence. In the absence of an electric field, droplets in the two streams do not in general arrive at the point of confluence at exactly the same time. When they do arrive synchronously the oil layer separating the droplets cannot drain quickly enough to facilitate coalescence and as a result the droplets do not coalesce. In contrast, upon application of an electric field, droplet formation becomes exactly synchronized, ensuring that droplets each reach the point of confluence simultaneously {i.e., paired droplets}.

Moreover, since the droplets are oppositely charged they are attracted to one another, which forces them to traverse the fluid stream lines and contact each other, thereby causing them to coalesce. The remarkable synchronization of the droplet formation results from coupling of the break-off of each of the pair of droplets as mediated by the electric field. The use of oppositely charged droplets and an electric field to combine and mix reagents is extremely robust, and 100% of the droplets coalesce with their partner from the opposite stream.

Other embodiments of the microfluidic devices of the present invention can include a droplet sorter. The contents of individual droplets must be probed, and selected droplets sorted into discreet streams. In one embodiment, such sorting in microfluidic devices can be accomplished through the use of mechanical valves. In another embodiment of the present invention, the use of electrostatic charging of droplets provides an alternate means that can be precisely controlled, can be switched at high frequencies, and requires no moving parts. Electrostatic charge on the droplets enables drop-by-drop sorting based on the linear coupling of charge to an external electric field. As an example, a T-junction bifurcation that splits the flow of carrier fluid equally will also randomly split the droplet population equally into the two streams. However, a small electric field applied at the bifurcation precisely dictates which channel the drops enter.

Varying the direction of the field varies the direction of the sorted droplets. The large forces that can be imparted on the droplets and the short time required to switch the field make this a fast and robust sorting engine with no moving parts; thus the processing rate is limited only by the rate of droplet generation and electric field switching time, and can easily exceed 20,000 per second.

Accordingly, in one embodiment the present invention provides a microfluidic device comprising a microfabricated substrate comprising at least one inlet channel adapted to carry at least one dispersed phase fluid and at least one main channel adapted to carry a continuous phase fluid, where inlet channel is in fluid communication with the main channel at one or more inlet modules such that the dispersed phase fluid is immiscible with the continuous phase fluid and forms a plurality of droplets in the continuous phase fluid; a coalescence module, where an electric field is applied to cause two or more droplets to coalesce; and c) a detection module including a detection apparatus for evaluating the contents and/or characteristics of the coalesced droplets produced in the coalescence module. The microfabricated substrate can further comprise one or more sorting modules, collection modules, waste modules, branch channels, delay modules, mixing modules and/or UV release modules, or any combinations thereof in any order. FIG. 1.

The present invention also provides methods of creating a nanoreactor. The method includes a) providing a microfabricated substrate comprising at least one inlet channel adapted to carry at least one dispersed phase fluid and at least one main channel adapted to carry a continuous phase fluid, where the inlet channel is in fluid communication with the main channel at one or more inlet modules, and where the dispersed phase fluid is immiscible with the continuous phase fluid; b) flowing a first dispersed phase fluid through a first inlet channel such that the first dispersed phase fluid forms one or more droplets in the continuous phase fluid; c) flowing at least a second dispersed phase fluid through an at least second inlet channel such that the second dispersed phase fluid forms one or more droplets in the continuous phase fluid; and d) coalescing at least one droplet formed in step (b) with at least one droplet formed in step (c) under the influence of an electric field, thereby producing a nanoreactor.

The present invention also provides a method for manipulating a nanoreactor. The method includes providing a nanoreactor as described herein; providing a plurality of electrically addressable channel bearing microfluidic modules integrally arranged with each other on a microfabricated substrate so as to be in fluid communication and providing a control system for manipulating the nanoreactor.

The present invention also provides methods of manipulating biological/chemical material. The method includes a) providing a microfabricated substrate comprising at least one inlet channel adapted to carry at least one dispersed phase fluid and at least one main channel adapted to carry a continuous phase fluid, where the inlet channel is in fluid communication with the main channel at one or more inlet modules, and where the dispersed phase fluid is immiscible with the continuous phase fluid; b) flowing a first dispersed phase fluid comprising a first biological/chemical material through a first inlet channel such that the first dispersed phase fluid resides as one or more droplets in the continuous phase fluid; c) flowing at least a second dispersed phase fluid comprising a second biological/chemical material through a second inlet channel such that the second dispersed phase fluid resides as one or more droplets in the continuous phase fluid; d) slowing or stopping at least one droplet formed in

step (b) by exerting a dielectrophoretic force onto the droplet; e) coalescing at least one droplet formed in step (c) with the droplet slowed or stopped in step (d) under the influence of an electric field within a coalescence module, thereby producing a nanoreactor; f) incubating the nanoreactor within a delay module; and g) interrogating the nanoreactor for a predetermined characteristic within a detection module. Slowing or stopping the droplets from step (b) allows pairing of the droplets from step (c) before they move to the location (e) where they are driven to coalesce by an electric field, or passively by passing through a narrowing of the channel.

In step (d), the pairing of droplets from (b) and (c) may be achieved in one of three ways: (i) using the dielectrophoretic force produced by the electric field gradient; (ii) using droplets of two different sizes, which works best when one droplet is comparable to the channel width and one droplet is smaller than the channel width, so that the smaller droplet catches up to the larger droplet; and (iii) the droplet in steps (b) and (c) have different viscosities, and thus, move at different velocities. Preferably, the droplets are of different sizes, and more preferably, the larger droplet has enough volume so that it would have a diameter greater than the channel width if it were spherical.

Methods of soiling biological/chemical material, although frequently desired, is not necessary in order to use the devices or practice the methods of the present invention. In particular, the devices and methods of the invention also include embodiments wherein the biological/chemical material is analyzed and/or identified, but is not sorted. The generation of nanoreactors through the coalescence of two droplets, although frequently desired, is not necessary in order to use the devices or practice the methods of the present invention. In particular, the devices and methods of the invention also include embodiments wherein the biological/chemical material is sorted without a coalescence event.

Substrates

The present invention also provides methods of producing a microfluidic device. The method of producing a microfluidic device comprises one or more of the following steps in any combination: 1) hard lithography, 2) soft lithography, 3) extraction and/or punch though, 4) bonding, 5) channel coating, 6) interconnect assembly, 7) electrode injection and 8) waveguide injection and fiber installation. The foregoing steps are described in more detail herein.

An "analysis unit" is a microfabricated substrate, e.g., a microfabricated chip, having at least one inlet channel, at least one main channel, at least one coalescence module, and at least one detection module. The analysis unit can further contain one or more sorting module. The sorting module can be in fluid communication with branch channels in communication with one or more outlet modules (collection module or waste module). For sorting, at least one detection module cooperates with at least one sorting module to divert flow via a detector-originated signal. It shall be appreciated that the "modules" and "channels" are in fluid communication with each other and therefore may overlap; i.e., there may be no clear boundary where a module or channel begins or ends. A device according to the invention may comprise a plurality of analysis units.

A variety of channels for sample flow and mixing can be microfabricated on a single chip and can be positioned at any location on the chip as the detection or sorting modules, e.g., for kinetic studies. A plurality of analysis units of the invention may be combined in one device. Microfabrication applied according to the invention eliminates the dead time

occurring in conventional gel electrophoresis or flow cytometric kinetic studies, and achieves a better time-resolution. Furthermore, linear arrays of channels on a single chip, i.e., a multiplex system, can simultaneously detect and sort a sample by using an array of photo multiplier tubes (PMT) for parallel analysis of different channels. This arrangement can be used to improve throughput or for successive sample enrichment, and can be adapted to provide a very high throughput to the microfluidic devices that exceeds the capacity permitted by conventional flow sorters. Circulation systems can be used in cooperation with these and other features of the invention. Positive displacement pressure driven flow is a preferred way of controlling fluid flow and electric fields and electric field gradients are a preferred way of manipulating droplets within that flow.

Microfabrication permits other technologies to be integrated or combined with flow cytometry on a single chip, such as PCR, moving cells using optical tweezer/cell trapping, transformation of cells by electroporation, μ TAS, and DNA hybridization. Detectors and/or light filters that are used to detect cellular characteristics of the reporters can also be fabricated directly on the chip. Preferably, detectors are off-chip free space optics or off-chip electronics with on-chip leads.

A device of the invention can be microfabricated with a sample solution reservoir or well or other apparatus for introducing a sample to the device, at the inlet module, which is typically in fluid communication with an inlet channel. A reservoir may facilitate introduction of molecules or cells into the device and into the sample inlet channel of each analysis unit. An inlet module may have an opening such as in the floor of the microfabricated chip, to permit entry of the sample into the device. The inlet module may also contain a connector adapted to receive a suitable piece of tubing, such as liquid chromatography or HPLC tubing, through which a sample may be supplied. Such an arrangement facilitates introducing the sample solution under positive pressure in order to achieve a desired infusion rate at the inlet module.

A microfabricated device of the invention is preferably fabricated from a silicon microchip or silicon elastomer. The dimensions of the chip are those of typical microchips, ranging between about 0.5 cm to about 7.5 cm per side and about 1 micron to about 1 cm in thickness. A microfabricated device can be transparent and can be covered with a material having transparent properties, such as a glass coverslip, to permit detection of a reporter, for example, by an optical device such as an optical microscope.

The device of the present invention can comprise inlet and outlet interconnects. The interconnections, including tubes, must be extremely clean and make excellent bonding with the PDMS surface in order to allow proper operation of the device. The difficulty in making a fluidic connection to a microfluidic device is primarily due to the difficulty in transitioning from a macroscopic fluid line into the device while minimizing dead volume. Development of a commercial microfluidic platform requires a simple, reliable fluidic interconnect in order to reduce the chance of operator and error leaks. The curing and manufacturing of the PDMS slab with the tubes already placed on the silicon wafer accomplish these goals.

The template process can include, but is not limited to, the following features. In order to minimize contamination and leakage, process operations that allow for greater reproducibility and reliability are improved. Tubes and interconnects for the PDMS slab can be cured in place. The tubes and interconnects can be placed in position by applying a

UV-cured adhesive to allow for holding the tubes in place on the silicon wafer. Once the tubes are placed in position, PDMS can be poured over the wafer and cured. The cured PDMS, along with the tubes in place, can be peeled off of the silicone wafer easily. This process can be applied to fluidics channels as well as other connection channels. Once the adhesive is applied onto the wafer, the process will allow for quick templating of PDMS slabs with exact reproducibility of channel locations and cleanliness. Tubes of any size can be implemented for this process. This process allows for less stress on the interconnection joints and smaller interconnection footprints in the device.

In one embodiment, small interconnects based on creating a face seal between the tubing and the device are used. A grommet may be placed into either a tapered hole or a hole with perpendicular walls. In one embodiment, the raised contact surface between the two sides is formed on the tubing side instead of the device side. In another embodiment, the sealing feature can be molded into the device. In yet another embodiment, a possible interconnect can be molded and bonded on a glass substrate directly from PDMS. In this embodiment, a thin film of PDMS can be simultaneously formed and bonded to the top of the glass slide and permits the use of isolated patterned electrodes and heating elements beneath the fluid channels. If not required, the seals could be made without the top skin. The raised contact surface could also be built into the tubing side. The sealing surface on the tubing side of the connection can be formed directly into the face of the tubing, although a separate piece secured to the tubing assembly/retaining nut may also be used.

The tubing side of the interconnect can be mounted into a retaining block that provides precise registration of the tubing, while the microfluidic device can be positioned accurately in a carrier that the retaining block would align and clamp to. The total dead volume associated with these designs would be critically dependent on how accurately the two mating surfaces could be positioned relative to each other, the maximum force required to maintain the seal would be limited by the exact shape and composition of the sealing materials as well as the rigidity and strength of the device itself. The shapes of the mating surfaces can be tailored to the minimal leakage potential, sealing force required, and potential for mis-alignment. By way of non-limiting example, the single ring used in the fluidic interconnects can be replaced with a series of rings of appropriate cross-sectional shape.

The device of the present invention can comprise a layer, such as a glass slide, which is perforated for functional interconnects, such as fluidic, electrical, and/or optical interconnects, and sealed to the back interface of the device so that the junction of the interconnects to the device is leak-proof. Such a device can allow for application of high pressure to fluid channels without leaking.

A silicon substrate containing the microfabricated flow channels and other components is preferably covered and sealed, most preferably with a transparent cover, e.g., thin glass or quartz, although other clear or opaque cover materials may be used. When external radiation sources or detectors are employed, the detection module is covered with a clear cover material to allow optical access to the cells. For example, anodic bonding to a "PYREX" cover slip can be accomplished by washing both components in an aqueous H_2SO_4/H_2O_2 bath, rinsing in water, and then, for example, heating to about 350° C. while applying a voltage of 450 V.

The present invention provides improved methods of bonding PDMS to incompatible media. Normal methods of bonding various materials (plastic, metals, etc) directly to materials such as PDMS, silicone, Teflon, and PEEK using traditional bonding practices (adhesives, epoxies, etc) do not work well due to the poor adhesion of the bonding agent to materials such as PDMS. Normal surface preparation by commercially available surface activators has not worked well in microfluidic device manufacturing. This problem is eliminated by treating the PDMS surface to be bonded with high intensity oxygen or air plasma. The process converts the top layer of PDMS to glass which bonds extremely well with normal adhesives. Tests using this method to bond external fluid lines to PDMS using a UV-cure adhesive (Loctite 352, 363, and others) resulted in a bond that is stronger than the PDMS substrate, resulting in fracture of the PDMS prior to failure of the bond. The present method combines high radiant flux, wavelength selection, and cure exposure time to significantly enhance the bond strength of the adhesive.

Channels

The invention provides microfluidic devices having channels that form the boundary for a fluid. The channels of the device carry a mixture of incompatible or immiscible fluids, such as an oil-water mixture. Droplets of aqueous solution containing a biological/chemical material are dispersed within the oil or other incompatible solvent. Each droplet of this multi-phase mixture can encapsulate one or more molecules, particles, or cells. The droplets are trapped and their boundaries are defined by channel walls, and therefore they do not diffuse and/or mix. Individual particles or molecules can be separately compartmentalized inside individual droplets. These droplets can be analyzed, combined with other droplets (e.g. to react droplet contents) and analyzed, and then sorted. Thus, the invention also provides methods for analyzing, combining, detecting and/or sorting of biological/chemical materials.

The channels present in the device can be made with micron dimensions and the volume of the detection module is precisely controlled. The planar geometry of the device allows the use of high numerical aperture optics, thereby increasing the sensitivity of the system. Because the system is entirely self-contained, there is no aerosol formation, allowing for much safer sorting of biohazardous materials. Materials sorted in the device are compartmentalized within individual droplets of an aqueous solution traveling in a flow of a second, incompatible or immiscible solution. Thus, there is no problem with the material diffusing or exchanging positions, even when sorting or analyzing extremely small particles, molecules, or reagents. In a preferred embodiment, water droplets are extruded into a flow of oil, but any fluid phase may be used as a droplet phase and any other incompatible or immiscible fluid or phase may be used as a barrier phase.

A "channel," as used herein, means a feature on or in a device (e.g., a substrate) that at least partially directs the flow of a fluid. In some cases, the channel may be formed, at least in part, by a single component, e.g., an etched substrate or molded unit. The channel can have any cross-sectional shape, for example, circular, oval, triangular, irregular, square or rectangular (having any aspect ratio), or the like, and can be covered or uncovered (i.e., open to the external environment surrounding the channel). In embodiments where the channel is completely covered, at least one portion of the channel can have a cross-section that is

completely enclosed, and/or the entire channel may be completely enclosed along its entire length with the exception of its inlet and outlet.

A channel may have an aspect ratio (length to average cross-sectional dimension) of at least 2:1, more typically at least 3:1, 5:1, or 10:1. As used herein, a "cross-sectional dimension," in reference to a fluidic or microfluidic channel, is measured in a direction generally perpendicular to fluid flow within the channel. An open channel generally will include characteristics that facilitate control over fluid transport, e.g., structural characteristics (an elongated indentation) and/or physical or chemical characteristics (hydrophobicity vs. hydrophilicity) and/or other characteristics that can exert a force (e.g., a containing force) on a fluid. The fluid within the channel may partially or completely fill the channel. In some cases the fluid may be held or confined within the channel or a portion of the channel in some fashion, for example, using surface tension (e.g., such that the fluid is held within the channel within a meniscus, such as a concave or convex meniscus). In an article or substrate, some (or all) of the channels may be of a particular size or less, for example, having a largest dimension perpendicular to fluid flow of less than about 5 mm, less than about 2 mm, less than about 1 mm, less than about 500 microns, less than about 200 microns, less than about 100 microns, less than about 60 microns, less than about 50 microns, less than about 40 microns, less than about 30 microns, less than about 25 microns, less than about 10 microns, less than about 3 microns, less than about 1 micron, less than about 300 nm, less than about 100 nm, less than about 30 nm, or less than about 10 nm or less in some cases. In one embodiment, the channel is a capillary. Of course, in some cases, larger channels, tubes, etc. can be used to store fluids in bulk and/or deliver a fluid to the channel.

In some embodiments, the dimensions of the channel may be chosen such that fluid is able to freely flow through the channel, for example, if the fluid contains cells. The dimensions of the channel may also be chosen, for example, to allow a certain volumetric or linear flow rate of fluid in the channel. Of course, the number of channels and the shape of the channels can be varied by any method known to those of ordinary skill in the art. In some cases, more than one channel or capillary may be used. For example, two or more channels may be used, where they are positioned inside each other, positioned adjacent to each other, etc.

A "main channel" is a channel of the device of the invention which permits the flow of molecules, cells, small molecules or particles past a coalescence module for coalescing one or more droplets, a detection module for detection (identification) or measurement or a droplet and a sorting module, if present, for sorting a droplet based on the detection in the detection module. The coalescence, detection and/or sorting modules can be placed or fabricated into the main channel. The main channel is typically in fluid communication with an inlet channel or inlet module. An "inlet channel" permits the flow of molecules, cells, small molecules or particles into the main channel. One or more inlet channels communicate with one or more means for introducing a sample into the device of the present invention. The inlet channel communicates with the main channel at an inlet module. The main channel is also typically in fluid communication with an outlet module and optionally with branch channels, each of which may have a collection module or waste module. These channels permit the flow of cells out of the main channel.

Channels of the device of the present invention can be formed from silicon elastomer (e.g. RTV), urethane com-

positions, of from silicon-urethane composites such as those available from Polymer Technology Group (Berkeley, Calif.), e.g. PurSil™ and CarboSil™. The channels may also be coated with additives or agents, such as surfactants, TEFLON, or fluorinated oils such as octadecafluorooctane 5 (98%, Aldrich), Fluorinert (FC-3283; 3M), or fluorononane, any of which can be modified to contain a fluorosurfactant. Fluorinated oils have favorable properties including chemical inertness, high gas permeability, and biocompatibility, which are desirable in microfluidic applications. TEFLON is particularly suitable for silicon elastomer (RTV) channels, which are hydrophobic and advantageously do not absorb water, but they may tend to swell when exposed to an oil phase. Swelling may alter channel dimensions and shape, and may even close off channels, or may affect the integrity of the chip, for example by stressing the seal between the elastomer and a coverslip. Urethane substrates do not tend to swell in oil but are hydrophilic, they may undesirably absorb water, and tend to use higher operating pressures. Hydrophobic coatings may be used to reduce or eliminate water absorption. Absorption or swelling issues may also be addressed by altering or optimizing pressure or droplet frequency (e.g. increasing periodicity to reduce absorption). RTV-urethane hybrids may be used to combine the hydrophobic properties of silicon with the hydrophilic properties of urethane. 25

The channels of the invention are microfabricated, for example by etching a silicon chip using conventional photolithography techniques, or using a micromachining technology called “soft lithography” as described by Whitesides and Xia, *Angewandte Chemie International Edition* 37, 550 (1998). These and other microfabrication methods may be used to provide inexpensive miniaturized devices, and in the case of soft lithography, can provide robust devices having beneficial properties such as improved flexibility, stability, 35 and mechanical strength. When optical detection is employed, the invention also provides minimal light scatter from molecule, cell, small molecule or particle suspension and chamber material. Devices according to the invention are relatively inexpensive and easy to set up. They can also be disposable, which greatly relieves many of the concerns of gel electrophoresis (for molecules), and of sterilization and permanent adsorption of particles into the flow chambers and channels of conventional FACS machines.

The channels of the device of the present invention can be of any geometry as described. However, the channels of the device can comprise a specific geometry such that the contents of the channel are manipulated, e.g., sorted, mixed, prevent clogging, etc. 45

For particles (e.g., cells) or molecules that are in droplets (i.e., deposited by the inlet module) within the flow of the main channel, the channels of the device are preferably rounded, with a diameter between about 2 and 100 microns, preferably about 60 microns, and more preferably about 30 microns at the cross-flow area or droplet extrusion region. This geometry facilitates an orderly flow of droplets in the channels. Similarly, the volume of the detection module in an analysis device is typically in the range of between about 10 femtoliters (fl) and 5000 fl, preferably about 40 or 50 fl to about 1000 or 2000 fl, most preferably on the order of about 200 fl. In preferred embodiments, the channels of the device, and particularly the channels of the inlet connecting to a droplet extrusion region, are between about 2 and 50 microns, most preferably about 30 microns. 60

A microfluidic device can include a bifurcation geometry designed in such a manner as to minimize fluidic shear forces on droplets during sorting. Known devices describe

bifurcation geometries in which significant shear forces affect droplets during sorting. Specifically droplets may experience shear forces when moving under the influence of the sorting force across the width of the input channel prior to encountering the bifurcation, and droplets may experience shear forces at the bifurcation point which are applied in such a manner as to elongate or even tear the droplet apart.

A microfluidic device comprising channels having a bifurcation geometry can minimize these shear forces by (i) including a necked-down segment of the input channel upstream of the bifurcation where the droplet is diagnosed to make the sorting decision, and/or by (ii) including a flared-out segment of the input channel immediately prior to the bifurcation, and/or by (iii) including a fork on the far wall of the bifurcation. The shear forces are minimized by component (i) because the sorting field is applied while the droplet is in the necked-down segment. Therefore, when the droplet exits the necked-down segment, the droplet is placed on fluid streamlines, which will carry it out the desired branch of the bifurcation. Furthermore, the droplet does not significantly encounter fluid streamlines, which follow the undesired branch of the bifurcation. The shear forces are minimized by component (ii) because the droplet does not significantly impact the far wall of the bifurcation at a point where it would experience fluid streamlines, which follow the undesired branch of the bifurcation. The shear forces are minimized by component (iii) because the fork serves to focus the two sets of fluid streamlines (i.e., the one set which follows one branch of the bifurcation, and the other set which follows the other branch of the bifurcation) away from each other. 30

A microfluidic device can include a specific geometry designed in such a manner as to prevent the aggregation of biological/chemical material and keep the biological/chemical material separated from each other prior to encapsulation in droplets. The geometry of channel dimension can be changed to disturb the aggregates and break them apart by various methods, that can include, but is not limited to, geometric pinching (to force cells through a (or a series of) narrow region(s), whose dimension is smaller or comparable to the dimension of a single cell) or a barricade (place a series of barricades on the way of the moving cells to disturb the movement and break up the aggregates of cells). 35

Channel design can force biological/chemical material moving along the center streamline through flow focus, e.g., using two dilution channels at the entrance of the channel to prevent attachment to the channel surface. This can also be used to prevent the surface attachment by cells. 45

Droplets at these dimensions tend to conform to the size and shape of the channels, while maintaining their respective volumes. Thus, as droplets move from a wider channel to a narrower channel they become longer and thinner, and vice versa. Droplets can be at least about four times as long as they are wide. This droplet configuration, which can be envisioned as a lozenge shape, flows smoothly and well through the channels. Longer droplets, produced in narrower channels, provides a higher shear, meaning that droplets can more easily be sheared or broken off from a flow, i.e. using less force. Droplets can also tend to adhere to channel surfaces, which can slow or block the flow, or produce turbulence. Droplet adherence is overcome when the droplet is massive enough in relation to the channel size to break free. Thus, droplets of varying size, if present, can combine to form uniform droplets having a so-called critical mass or volume that results in smooth or laminar droplet flow. Droplets that are longer than they are wide, preferably about four times longer than they are wide, generally have the 65

ability to overcome channel adherence and move freely through the microfluidic device. Thus, in an exemplary embodiment with 60 micron channels, a typical free-flowing droplet is about 60 microns wide and 240 microns long. Droplet dimensions and flow characteristics can be influenced as desired, in part by changing the channel dimensions, e.g. the channel width.

The microfabricated devices of this invention most preferably generate round, monodisperse droplets. The droplets can have a diameter that is smaller than the diameter of the microchannel; i.e., preferably 40 to 100 μm when cells are used or 5 to 40 μm when reagents are used. Monodisperse droplets may be particularly preferably, e.g., in high throughput devices and other embodiments where it is desirable to generate droplets at high frequency and of high uniformity.

To prevent material (e.g., cells and other particles or molecules) from adhering to the sides of the channels, the channels (and coverslip, if used) may have a coating which minimizes adhesion. Such a coating may be intrinsic to the material from which the device is manufactured, or it may be applied after the structural aspects of the channels have been microfabricated. "TEFLON" is an example of a coating that has suitable surface properties.

The surface of the channels of the microfluidic device can be coated with any anti-wetting or blocking agent for the dispersed phase. The channel can be coated with any protein to prevent adhesion of the biological/chemical sample. For example, in one embodiment the channels are coated with BSA, PEG-silane and/or fluorosilane. For example, 5 mg/ml BSA is sufficient to prevent attachment and prevent clogging. In another embodiment, the channels can be coated with a cyclized transparent optical polymer obtained by copolymerization of perfluoro (alkenyl vinyl ethers), such as the type sold by Asahi Glass Co. under the trademark Cytop. In such an embodiment, the coating is applied from a 0.1-0.5 wt % solution of Cytop CTL-809M in CT-SoIv 180. This solution can be injected into the channels of a microfluidic device via a plastic syringe. The device can then be heated to about 90° C. for 2 hours, followed by heating at 200° C. for an additional 2 hours. In another embodiment, the channels can be coated with a hydrophobic coating of the type sold by PPG Industries, Inc. under the trademark Aquapel (e.g., perfluoroalkylalkylsilane surface treatment of plastic and coated plastic substrate surfaces in conjunction with the use of a silica primer layer) and disclosed in U.S. Pat. No. 5,523,162, which patent is hereby incorporated by reference. By fluorinating the surfaces of the channels, the continuous phase preferentially wets the channels and allows for the stable generation and movement of droplets through the device. The low surface tension of the channel walls thereby minimizes the accumulation of channel clogging particulates.

The surface of the channels in the microfluidic device can be also fluorinated to prevent undesired wetting behaviors. For example, a microfluidic device can be placed in a polycarbonate dessicator with an open bottle of (tridecafluoro-1,1,2,2-tetrahydrooctyl)trichlorosilane. The dessicator is evacuated for 5 minutes, and then sealed for 20-40 minutes. The dessicator is then backfilled with air and removed. This approach uses a simple diffusion mechanism to enable facile infiltration of channels of the microfluidic device with the fluorosilane and can be readily scaled up for simultaneous device fluorination.

The microfluidic device can include a syringe (or other glass container) that is treated with a vapor or solution of an appropriate PEG-silane to effect the surface PEG function-

alization. The purpose for treating the walls of glass containers (e.g., syringes) with a PEG functionality is to prevent biological adhesion to the inner walls of the container, which frustrates the proper transfer of biological/chemical materials into the microfluidic device of the present invention.

The device of the present invention can comprise one or more fluid channels to inject or remove fluid in between droplets in a droplet stream for the purpose of changing the spacing between droplets.

The invention provides methods of cell manipulation by channel geometry. Most cells, especially mammalian cells intend to attach each other in suspension. The purpose of changing channel geometry is to detach the cell from aggregates and keep them separated from each other before they are encapsulated in the drops. The geometry of channel dimension can be changed to disturb the aggregates and break them apart by various methods, that can include, for example, geometric pinching and/or barricades. With geometric pinching, cells are forced through one or more narrow regions, whose dimension is smaller or comparable to the dimension of a single cell. With a barricade, a series of obstacles/impediments (barricades) are placed in the way of the moving cells to disturb the movement and break up the aggregates of cells.

The present invention provides methods to prevent channel clogging including methods of fluid pinching and surface coating. Some cells and polystyrene beads tend to attach to the PDMS/Glass surface. This is an undesired result as the accumulated beads can clog the channel, especially the narrow region (i.e. nozzle). Channel design and blocking reagent can be used in some embodiments to prevent the beads' attachment to the channel surface and to each other. Non-limiting examples include coating reagents and channel design. A coating reagent, such as BSA (or any other protein), is added to the bead buffer to coat the channel surface as well as the beads' surface. 5 mg/ml BSA has shown to be sufficient to prevent the beads' attachment. No clogging is observed in an experiment with 1 μm diameter beads in a 30 μm wide and 25 μm deep nozzle device. With channel design, cells/beads are forced to move along the center streamline through flow focus—Using two dilution channels at the entrance of the beads' channel to prevent beads' attachment to the channel surface. This can also used to prevent the surface attachment by cells.

A typical analysis unit of the invention comprises a main inlet channel that is part of and feeds or communicates directly with a main channel, along with one or more sample inlet channels in communication with the main channel at a inlet module situated downstream from the main inlet. In one embodiment, each different sample inlet channel preferably communicates with the main channel at a different inlet module. In another embodiment, different sample inlet channels can communicate with the main channel at the same inlet module. The inlet channel is further connected to a means for introducing a sample to said device. The means can be a well or reservoir. The well or reservoir further include an acoustic actuator. The means can be temperature controlled. The main channel is further connected to a means for collecting a sample from said device. The means can be a well or reservoir. The means can be temperature controlled.

The inlet module generally comprises a junction between the sample inlet channel and the main channel such that a solution of a sample (i.e., a fluid containing a sample such as molecules, cells, small molecules (organic or inorganic) or particles) is introduced to the main channel and forms a plurality of droplets. The sample solution can be pressur-

ized. The sample inlet channel can intersect the main channel such that the sample solution is introduced into the main channel at an angle perpendicular to a stream of fluid passing through the main channel. For example, the sample inlet channel and main channel intersect at a T-shaped junction; 5 i.e., such that the sample inlet channel is perpendicular (90 degrees) to the main channel. However, the sample inlet channel can intercept the main channel at any angle, and need not introduce the sample fluid to the main channel at an angle that is perpendicular to that flow. The angle between 10 intersecting channels is in the range of from about 60 to about 120 degrees. Particular exemplary angles are 45, 60, 90, and 120 degrees.

The main channel in turn can communicate with two or more branch channels at the sorting module or “branch point”, if present, forming, for example, a T-shape or a Y-shape. Other shapes and channel geometries may be used as desired. 15

The device of the present invention can comprise one more means for chromatographically sorting the sample prior to droplet formation. The means can be in fluid communication with the inlet channel and/or the inlet module. Preferably, the means is a channel. The sample can be sorted by size, charge, hydrophobicity, atomic mass, etc. The separating can be done isocratic or by generating a gradient 20 chemically, (for example using salt or hydrophobicity), electrically, by pressure, or etc. For size exclusion, the channel can be preloaded with Sepharose. The sample is then loaded at one end, and the droplets are formed at an opposing end. The sample separates by size prior to becoming 25 incorporated within a droplet.

Fluids

The term “flow” means any movement of liquid or solid through a device or in a method of the invention, and encompasses without limitation any fluid stream, and any material moving with, within or against the stream, whether or not the material is carried by the stream. For example, the movement of molecules, beads, cells or virions through a device or in a method of the invention, e.g. through channels of a microfluidic chip of the invention, comprises a flow. 30 This is so, according to the invention, whether or not the molecules, beads, cells or virions are carried by a stream of fluid also comprising a flow, or whether the molecules, cells or virions are caused to move by some other direct or indirect force or motivation, and whether or not the nature of any motivating force is known or understood. The application of any force may be used to provide a flow, including without limitation, pressure, capillary action, electro-osmosis, electrophoresis, dielectrophoresis, optical tweezers, and combinations thereof, without regard for any particular 35 theory or mechanism of action, so long as molecules, cells or virions are directed for detection, measurement or sorting according to the invention.

The flow stream in the main channel is typically, but not necessarily, continuous and may be stopped and started, reversed or changed in speed. Prior to sorting, a liquid that does not contain sample molecules, cells or particles can be introduced into a sample inlet well or channel and directed through the inlet module, e.g., by capillary action, to hydrate and prepare the device for use. Likewise, buffer or oil can 40 also be introduced into a main inlet region that communicates directly with the main channel to purge the device (e.g., or “dead” air) and prepare it for use. If desired, the pressure can be adjusted or equalized, for example, by adding buffer or oil to an outlet module.

The pressure at the inlet module can also be regulated by adjusting the pressure on the main and sample inlet chan-

nels, for example, with pressurized syringes feeding into those inlet channels. By controlling the pressure difference between the oil and water sources at the inlet module, the size and periodicity of the droplets generated may be regulated. Alternatively, a valve may be placed at or coincident 5 to either the inlet module or the sample inlet channel connected thereto to control the flow of solution into the inlet module, thereby controlling the size and periodicity of the droplets. Periodicity and droplet volume may also 10 depend on channel diameter, the viscosity of the fluids, and shear pressure.

As used herein, the term “fluid stream” or “fluidic stream” refers to the flow of a fluid, typically generally in a specific direction. The fluidic stream may be continuous and/or 15 discontinuous. A “continuous” fluidic stream is a fluidic stream that is produced as a single entity, e.g., if a continuous fluidic stream is produced from a channel, the fluidic stream, after production, appears to be contiguous with the channel outlet. The continuous fluidic stream is also referred to as a continuous phase fluid or carrier fluid. The continuous 20 fluidic stream may be laminar, or turbulent in some cases. The continuous fluidic stream may be, e.g., solid or hollow (i.e., containing a second fluid internally, for example, as in a hollow tube). It is to be understood that wherever “tube” 25 is used herein, the structure can be a hollow, a solid or filled (i.e., not hollow) stream, a stream that includes a central core and a surrounding layer or layers, any of which can be selectively reacted with any others, or solidified, or the like. In some cases, the central core is hollow, and/or fluid may 30 be removed from a hardened surrounding fluid to produce a hollow tube. The continuous phase fluid can be a non-polar solvent. The continuous phase fluid can be a fluorocarbon oil.

Similarly, a “discontinuous” fluidic stream is a fluidic stream that is not produced as a single entity. The discontinuous fluidic stream is also referred to as the dispersed phase fluid or sample fluid. A discontinuous fluidic stream may have the appearance of individual droplets, optionally 35 surrounded by a second fluid. A “droplet,” as used herein, is an isolated portion of a first fluid that completely surrounded by a second fluid. In some cases, the droplets may be spherical or substantially spherical; however, in other cases, the droplets may be non-spherical, for example, the droplets may have the appearance of “blobs” or other irregular 40 shapes, for instance, depending on the external environment. As used herein, a first entity is “surrounded” by a second entity if a closed loop can be drawn or idealized around the first entity through only the second entity. The dispersed phase fluid can include a biological/chemical material. The 45 biological/chemical material can be tissues, cells, particles, proteins, antibodies, amino acids, nucleotides, small molecules, and pharmaceuticals. The biological/chemical material can include one or more labels. The label can be a DNA tag, dyes or quantum dot, or combinations thereof.

The term “emulsion” refers to a preparation of one liquid distributed in small globules (also referred to herein as drops, droplets or NanoReactors) in the body of a second liquid. The first and second fluids are immiscible with each other. For example, the discontinuous phase can be an aqueous solution and the continuous phase can a hydrophobic fluid such as an oil. This is termed a water in oil emulsion. Alternatively, the emulsion maybe a oil in water emulsion. In that example, the first liquid, which is dispersed in globules, is referred to as the discontinuous phase, 50 whereas the second liquid is referred to as the continuous phase or the dispersion medium. The continuous phase can be an aqueous solution and the discontinuous phase is a 65

hydrophobic fluid, such as an oil (e.g., decane, tetradecane, or hexadecane). The droplets or globules of oil in an oil in water emulsion are also referred to herein as “micelles”, whereas globules of water in a water in oil emulsion may be referred to as “reverse micelles”.

As used herein, the term “NanoReactor” and its plural encompass the terms “droplet”, “microdrop” or “microdroplet” as defined herein, as well as an integrated system for the manipulation and probing of droplets, as described in detail herein. Nanoreactors as described herein can be 0-100 μm (e.g., 5, 10, 15, 20, 25, 30, 35, 40, 45, 50, 55, 60, 65, 70, 75, 80, 85, 90, 95, 100)

The droplet forming liquid is typically an aqueous buffer solution, such as ultrapure water (e.g., 18 mega-ohm resistivity, obtained, for example by column chromatography), 10 mM Tris HCl and 1 mM EDTA (TE) buffer, phosphate buffer saline (PBS) or acetate buffer. Any liquid or buffer that is physiologically compatible with the population of molecules, cells or particles to be analyzed and/or sorted can be used. The fluid passing through the main channel and in which the droplets are formed is one that is immiscible with the droplet forming fluid. The fluid passing through the main channel can be a non-polar solvent, most preferably decane (e.g., tetradecane or hexadecane), fluorocarbon oil or another oil (for example, mineral oil).

The dispersed phase fluid may also contain biological/chemical material (e.g., molecules, cells, or other particles) for combination, analysis and/or sorting in the device. The droplets of the dispersed phase fluid can contain more than one particle or can contain no more than one particle. For example, where the biological material comprises cells, each droplet preferably contains, on average, no more than one cell. The droplets can be detected and/or sorted according to their contents.

The fluids used in the invention may contain one or more additives, such as agents which reduce surface tensions (surfactants). Surfactants can include Tween, Span, fluorosurfactants, and other agents that are soluble in oil relative to water. Surfactants can aid in controlling or optimizing droplet size, flow and uniformity, for example by reducing the shear force needed to extrude or inject droplets into an intersecting channel. This can affect droplet volume and periodicity, or the rate or frequency at which droplets break off into an intersecting channel. Furthermore, the surfactant can serve to stabilize aqueous emulsions in fluorinated oils from coalescing.

The droplets may be coated with a surfactant. Preferred surfactants that may be added to the continuous phase fluid include, but are not limited to, surfactants such as sorbitan-based carboxylic acid esters (e.g., the “Span” surfactants, Fluka Chemika), including sorbitan monolaurate (Span 20), sorbitan monopalmitate (Span 40), sorbitan monostearate (Span 60) and sorbitan monooleate (Span 80), and perfluorinated polyethers (e.g., DuPont Krytox 157 FSL, FSM, and/or FSH). Other non-limiting examples of non-ionic surfactants which may be used include polyoxyethylenated alkylphenols (for example, nonyl-, p-dodecyl-, and dinonylphenols), polyoxyethylenated straight chain alcohols, polyoxyethylenated polyoxypropylene glycols, polyoxyethylenated mercaptans, long chain carboxylic acid esters (for example, glyceryl and polyglycerol esters of natural fatty acids, propylene glycol, sorbitol, polyoxyethylenated sorbitol esters, polyoxyethylene glycol esters, etc.) and alkanolamines (e.g., diethanolamine-fatty acid condensates and isopropanolamine-fatty acid condensates). In addition, ionic surfactants such as sodium dodecyl sulfate (SDS) may also be used. However, such surfactants are generally less pref-

erably for many embodiments of the invention. For instance, in those embodiments where aqueous droplets are used as nanoreactors for chemical reactions (including biochemical reactions) or are used to analyze and/or sort biomaterials, a water soluble surfactant such as SDS may denature or inactivate the contents of the droplet.

The carrier fluid can be an oil (e.g., decane, tetradecane or hexadecane) or fluorocarbon oil that contains a surfactant (e.g., a non-ionic surfactant such as a Span surfactant) as an additive (preferably between about 0.2 and 5% by volume, more preferably about 2%). A user can preferably cause the carrier fluid to flow through channels of the microfluidic device so that the surfactant in the carrier fluid coats the channel walls. In one embodiment, the fluorosurfactant can be prepared by reacting the perfluorinated polyether DuPont Krytox 157 FSL, FSM, or FSH with aqueous ammonium hydroxide in a volatile fluorinated solvent. The solvent and residual water and ammonia can be removed with a rotary evaporator. The surfactant can then be dissolved (e.g., 2.5 wt %) in a fluorinated oil (e.g., Fluorinert (3M)), which then serves as the continuous phase of the emulsion.

The invention can use pressure drive flow control, e.g., utilizing valves and pumps, to manipulate the flow of cells, particles, molecules, enzymes or reagents in one or more directions and/or into one or more channels of a microfluidic device. However, other methods may also be used, alone or in combination with pumps and valves, such as electroosmotic flow control, electrophoresis and dielectrophoresis (Fulwyer, *Science* 156, 910 (1974); Li and Harrison, *Analytical Chemistry* 69, 1564 (1997); Fiedler, et al. *Analytical Chemistry* 70, 1909-1915 (1998); U.S. Pat. No. 5,656,155). Application of these techniques according to the invention provides more rapid and accurate devices and methods for analysis or sorting, for example, because the sorting occurs at or in a sorting module that can be placed at or immediately after a detection module. This provides a shorter distance for molecules or cells to travel, they can move more rapidly and with less turbulence, and can more readily be moved, examined, and sorted in single file, i.e., one at a time.

Without being bound by any theory, electro-osmosis is believed to produce motion in a stream containing ions e.g. a liquid such as a buffer, by application of a voltage differential or charge gradient between two or more electrodes. Neutral (uncharged) molecules or cells can be carried by the stream. Electro-osmosis is particularly suitable for rapidly changing the course, direction or speed of flow. Electrophoresis is believed to produce movement of charged objects in a fluid toward one or more electrodes of opposite charge, and away from one or more electrodes of like charge. Where an aqueous phase is combined with an oil phase, aqueous droplets are encapsulated or separated from each other by oil. Typically, the oil phase is not an electrical conductor and may insulate the droplets from the electroosmotic field. In this example, electro-osmosis may be used to drive the flow of droplets if the oil is modified to carry or react to an electrical field, or if the oil is substituted for another phase that is immiscible in water but which does not insulate the water phase from electrical fields.

Dielectrophoresis is believed to produce movement of dielectric objects, which have no net charge, but have regions that are positively or negatively charged in relation to each other. Alternating, non-homogeneous electric fields in the presence of droplets and/or particles, such as cells or molecules, cause the droplets and/or particles to become electrically polarized and thus to experience dielectrophoretic forces. Depending on the dielectric polarizability of the particles and the suspending medium, dielectric particles

will move either toward the regions of high field strength or low field strength. For example, the polarizability of living cells depends on their composition, morphology, and phenotype and is highly dependent on the frequency of the applied electrical field. Thus, cells of different types and in different physiological states generally possess distinctly different dielectric properties, which may provide a basis for cell separation, e.g., by differential dielectrophoretic forces. Likewise, the polarizability of droplets also depends upon their size, shape and composition. For example, droplets that contain salts can be polarized. According to formulas provided in Fiedler, et al. *Analytical Chemistry* 70, 1909-1915 (1998), individual manipulation of single droplets requires field differences (inhomogeneities) with dimensions close to the droplets.

Manipulation is also dependent on permittivity (a dielectric property) of the droplets and/or particles with the suspending medium. Thus, polymer particles, living cells show negative dielectrophoresis at high-field frequencies in water. For example, dielectrophoretic forces experienced by a latex sphere in a 0.5 MV/m field (10 V for a 20 micron electrode gap) in water are predicted to be about 0.2 piconewtons (pN) for a 3.4 micron latex sphere to 15 pN for a 15 micron latex sphere (Fiedler, et al. *Analytical Chemistry* 70, 1909-1915 (1998)). These values are mostly greater than the hydrodynamic forces experienced by the sphere in a stream (about 0.3 pN for a 3.4 micron sphere and 1.5 pN for a 15 micron sphere). Therefore, manipulation of individual cells or particles can be accomplished in a streaming fluid, such as in a cell sorter device, using dielectrophoresis. Using conventional semiconductor technologies, electrodes can be microfabricated onto a substrate to control the force fields in a microfabricated sorting device of the invention. Dielectrophoresis is particularly suitable for moving objects that are electrical conductors. The use of AC current is preferred, to prevent permanent alignment of ions. Megahertz frequencies are suitable to provide a net alignment, attractive force, and motion over relatively long distances. See U.S. Pat. No. 5,454,472.

Radiation pressure can also be used in the invention to deflect and move objects, e.g. droplets and particles (molecules, cells, particles, etc.) contained therein, with focused beams of light such as lasers. Flow can also be obtained and controlled by providing a pressure differential or gradient between one or more channels of a device or in a method of the invention.

Molecules, cells or particles (or droplets containing molecules, cells or particles) can be moved by direct mechanical switching, e.g., with on-off valves or by squeezing the channels. Pressure control may also be used, for example, by raising or lowering an output well to change the pressure inside the channels on the chip. See, e.g., the devices and methods described U.S. Pat. No. 6,540,895. These methods and devices can further be used in combination with the methods and devices described in pending U.S. Patent Application Publication No. 20010029983 and 20050226742. The "pump and valve" drive systems are particularly preferred. They are rapid, efficient, economical, and relatively easy to fabricate and control. Additionally, they do not rely on electrical fields or electrical charges, which may be harder to control and in some cases may potentially affect the droplet contents. Different switching and flow control mechanisms can be combined on one chip or in one device and can work independently or together as desired.

The device can exchange constituents within a droplet through the use of fluid flow in such a way that the droplet,

while in a first immiscible fluid, is exposed to a second immiscible fluid such that constituents within the droplet that are immiscible in the first immiscible fluid are soluble in the second immiscible fluid. In one example, an aqueous droplet containing a chemical reaction produces by-products that are soluble in a lipid solvent. The chemical reaction is performed in a water-environment in a silicon-based solvent. After the chemical reaction occurs, the droplet is exposed to an organic-oil based solvent where the chemical byproducts are allowed to diffuse out of the droplet. The resulting droplet is then assayed for cell-killing activity by combining the droplet with live cells. Alternatively, the change in the non-aqueous fluid flow is used to add a particular constituent from the second immiscible fluid to diffuse into the aqueous drop before the droplet is returned to the 100% first immiscible fluid flow.

The concentration (i.e., number) of molecules, cells or particles in a droplet can influence sorting efficiently and therefore is preferably optimized. In particular, the sample concentration should be dilute enough that most of the droplets contain no more than a single molecule, cell or particle, with only a small statistical chance that a droplet will contain two or more molecules, cells or particles. This is to ensure that for the large majority of measurements, the level of reporter measured in each droplet as it passes through the detection module corresponds to a single molecule, cell or particle and not to two or more molecules, cells or particles.

The parameters which govern this relationship are the volume of the droplets and the concentration of molecules, cells or particles in the sample solution. The probability that a droplet will contain two or more molecules, cells or particles ($P_{\leq 2}$) can be expressed as

$$P_{\leq 2} = 1 - \{1 + [\text{cell}] \times V\} \times e^{-[\text{cell}] \times V}$$

where "[cell]" is the concentration of molecules, cells or particles in units of number of molecules, cells or particles per cubic micron (μm^3), and V is the volume of the droplet in units of μm^3 .

It will be appreciated that $P_{\leq 2}$ can be minimized by decreasing the concentration of molecules, cells or particles in the sample solution. However, decreasing the concentration of molecules, cells or particles in the sample solution also results in an increased volume of solution processed through the device and can result in longer run times. Accordingly, it is desirable to minimize to presence of multiple molecules, cells or particles in the droplets (thereby increasing the accuracy of the sorting) and to reduce the volume of sample, thereby permitting a sorted sample in a reasonable time in a reasonable volume containing an acceptable concentration of molecules, cells or particles.

The maximum tolerable $P_{\leq 2}$ depends on the desired "purity" of the sorted sample. The "purity" in this case refers to the fraction of sorted molecules, cells or particles that possess a desired characteristic (e.g., display a particular antigen, are in a specified size range or are a particular type of molecule, cell or particle). The purity of the sorted sample is inversely proportional to $P_{\leq 2}$. For example, in applications where high purity is not needed or desired a relatively high $P_{\leq 2}$ (e.g., $P_{\leq 2} = 0.2$) may be acceptable. For most applications, maintaining $P_{\leq 2}$ at or below about 0.1, preferably at or below about 0.01, provides satisfactory results.

A sample solution containing a mixture or population of molecule, cells or particles in a suitable fluid (such as a liquid or buffer described above) is supplied to the sample inlet channel, and droplets of the sample solution are introduced, at the inlet module, into the flow passing through the

main channel. The force and direction of flow can be controlled by any desired method for controlling flow, for example, by a pressure differential, by valve action or by electro-osmotic flow (e.g., produced by one or more electrodes or patterned electrically conductive layers at inlet and/or outlet modules). This permits the movement of the cells into one or more desired branch channels or outlet modules.

Both the fluid comprising the droplets and the fluid carrying the droplets (i.e., the aqueous and non-polar fluids) have, preferably, a relatively low Reynolds Number, for example 10^{-2} . The Reynolds Number represents an inverse relationship between the density and velocity of a fluid and its viscosity in a channel of given length. More viscous, less dense, slower moving fluids over a shorter distance will have a lower Reynolds Number, and are easier to divert, stop, start, or reverse without turbulence. Because of the small sizes and slow velocities, microfabricated fluid systems are often in a low Reynolds number regime ($Re \ll 1$). In this regime, inertial effects, which cause turbulence and secondary flows, are negligible; viscous effects dominate the dynamics. These conditions are advantageous for sorting, and are provided by microfabricated devices of the invention. Accordingly the microfabricated devices of the invention are preferably if not exclusively operated at a low or very low Reynold's number.

The device of the present invention can be used to generate droplets whose composition may vary from one droplet to the next droplet due to any number of reasons (chemical reaction, sample preparation, etc). Within the same device, the droplets can be passed through a measurement volume in which the contents can be interrogated using various means (optical or electrical). The result of the measurement can be used to decide which flow path the droplets should take. The means of changing the flow path can be accomplished through mechanical, electrical, optical, or other technique as described herein or well known in the art.

The present invention provides methods for the determination of droplet size and rate information without the need for optical measurements on a microfluidic device. The need to control the timing between multiple events requires the determination of the exact time when a droplet passes a given point. It is also essential to know which channel a droplet enters. This method can significantly reduce the cost and complexity of such measurements.

The fluids used to generate droplets in microfluidic devices are typically immiscible liquids such as oil and water. These two materials generally have very different dielectric constants associated with them. These differences can be exploited to determine droplet rate and size for every drop passing through a small section of a microfluidic device. One method to directly monitor this variation in the dielectric constant measures the change in capacitance over time between a pair of closely spaced electrodes. This change in capacitance can be detected by the change in current measured in these electrodes:

$$i = V \frac{dC}{dt}$$

Where i is the current, V is the voltage applied across the electrodes, and dC/dt is the change in capacitance with time. Alternatively, the capacitance can be measured directly if a time varying voltage is applied to these same electrodes:

$i = CdV/dt$ Where C is the measured capacitance, and dV/dt is the change in voltage with time.

As a first approximation, the electrode pair can be determined as a parallel plate capacitor:

$$C = \epsilon_0 k \frac{A}{d}$$

Where ϵ_0 is the permittivity of free space, k is the effective dielectric constant (this changes every time a droplet passes through), A is the area of the capacitor and d is the electrode separation. The current measured in the device is then plotted as a function of time.

Inlet Module

An "inlet module" is an area of a microfabricated device that receives molecules, cells, small molecules or particles for coalescence, detection and/or sorting. The inlet module can contain one or more inlet channels, wells or reservoirs, openings, and other features which facilitate the entry of molecules, cells, small molecules or particles into the device. A chip may contain more than one inlet module if desired. The inlet module is in fluid communication with the main channel. The inlet module can include a junction between an inlet channel and the main channel of a device of the invention. The junction can permit the introduction of a pressurized fluid to the main channel. The inlet channel can be at an angle perpendicular to the flow of fluid in the main channel. The fluid introduced to the main channel through the inlet module is "incompatible" (i.e., immiscible) with the fluid in the main channel so that droplets of the fluid introduced through the inlet module are formed in the stream of continuous fluid in the main channel.

Embodiments of the invention are also provided in which there are two or more inlet modules introducing droplets of samples into the main channel. For example, a first inlet module may introduce droplets of a first sample into a flow of fluid (e.g., oil) in the main channel and a second inlet module may introduce droplets of a second sample into the flow of fluid in main channel, and so forth. The second inlet module is preferably downstream from the first inlet module (e.g., about 30 μm). The fluids introduced into the two or more different inlet modules can comprise the same fluid or the same type of fluid (e.g., different aqueous solutions). For example, droplets of an aqueous solution containing an enzyme are introduced into the main channel at the first inlet module and droplets of aqueous solution containing a substrate for the enzyme are introduced into the main channel at the second inlet module. Alternatively, the droplets introduced at the different inlet modules may be droplets of different fluids which may be compatible or incompatible. For example, the different droplets may be different aqueous solutions, or droplets introduced at a first inlet module may be droplets of one fluid (e.g., an aqueous solution) whereas droplets introduced at a second inlet module may be another fluid (e.g., alcohol or oil).

To obtain one droplet comprising a single element of a specific biological/chemical material (e.g., a cell), separation of biological/chemical material, and uniformity of the number density of biological/chemical materials in a microfluidic channel is desirable. Accordingly, the microfluidic device can include an acoustic actuator. The loaded sample (biological/chemical material) can be well mixed and separated in a small chamber by acoustic wave before sending out to the nozzle region for encapsulation. The frequency of the acoustic wave should be fine tuned so as not to cause any

damage to the cells. The biological effects of acoustic mixing have been well studied (e.g., in the ink-jet industry) and many published literatures also showed that piezoelectric microfluidic device can deliver intact biological payloads such as live microorganisms and DNA.

The design of the acoustic resonant can use a Piezoelectric bimorph flat plate located on the side of the carved resonant in the PDMS slab. The resonant inlet can connect to the cell flow input channel and the outlet can connect to the cell flow pinching channel. The piezoelectric driving waveform can be carefully optimized to select the critical frequencies that can separate cells in fluids. There are five parameters to optimize beyond the frequency parameter and Lab electronics can be used to optimize the piezoelectric driving waveform. Afterwards, a low cost circuit can be designed to generate only the optimized waveform in a preferred microfluidic device.

Coalescence Module

The device of the invention also comprises one or more coalescence modules. A "coalescence module" is within or coincident with at least a portion of the main channel at or downstream of the inlet module where molecules, cells, small molecules or particles comprised within droplets are brought within proximity of other droplets comprising molecules, cells, small molecules or particles and where the droplets in proximity coalesce or combine their contents. The coalescence module can also include an apparatus, preferably one or more electrodes or patterned electrically conductive layers for generating a dielectrophoretic force. The dielectrophoretic force generated by one or more electrodes or patterned electrically conductive layers can slow or stop the droplets within the main channel thereby facilitating their proximity and resulting coalescence or combination.

Two or more precursor droplets in one or more droplet streams can be coalesced into a larger droplet by applying a voltage to produce an electric field. The voltage can be alternating. The electric field can be an AC electric field, or a DC electric field.

The coalescing influence can create a dielectrophoretic force that slows or stops a first precursor droplet relative to the velocity of the stream that carries the droplet. The first precursor droplet will remain slow or stopped until a second (or more) precursor droplet arrives and coalesces with the first precursor droplet due to interactions between the field induced dipoles in the droplets. The new droplet of increased volume is then too large to be held by the dielectric field and moves off under the influence of the flow of the continuous phase fluid. See FIGS. 15-17. No change in the applied voltage is required and the electric field remains constant. Both the trapping (slowing or stopping) of the precursor droplets and the release of the coalesced droplet can be passive. Once the new droplet of increased volume moves off, the next precursor droplet is then trapped in the field and the process repeated. The voltage can be tuned such that more than one droplet is coalesced with a trapped droplet. An advantage of coalescing more than one droplet with another is that it allows for pairwise combinations. Alternatively, a variation on this geometry will allow precise control of the droplet phase by temporarily shifting droplets to low velocity streamlines in the flow.

The precursor droplets can come at different times in the same fluid stream and subsequently coalesce. Alternatively, the precursor droplets can arrive together in different (e.g., two or more) fluid streams so that the droplets are in a substantially adjacent position with respect to each other when they come under the influence of the dielectrophoretic force and then subsequently coalesce due to the interactions

between the field induced dipoles in the droplets. The different fluid streams can be substantially parallel.

The electric field gradient can be stronger for precursor droplets in a first parallel fluid stream than for precursor droplets in a second (or more) parallel fluid stream. Accordingly, it is only the precursor droplets from the first stream that are trapped, thereby preventing coalescence of precursor droplets in the other fluid stream(s) among each other in the case where the frequency of precursor droplets in the other stream(s) is greater than the frequency of precursor droplets in the first stream. In this manner the electric field can be changed to cause coalescence of only correct pairs of precursor droplets. Thus, in some embodiments the trapping and release of the droplets can be non-passive (i.e., based on whether the electric field is on or off).

The device can include channels for use in fluid control and other channels filled with a metal alloy for casting integrated metal alloy components (i.e., electrodes). Alternatively, the electrodes can be manufactured using other technologies (e.g., lithographically patterned electrodes made from indium tin oxide or a metal such as platinum). The microfluidic device can include metal alloy components useful for performing electrical functions on fluids, including but not limited to, coalescing droplets, charging droplets, sorting droplets, detecting droplets and shaking droplets to mix the contents of coalesced droplets. The device can contain more than one of the above mentioned components for more than one of the above mentioned functions.

The present invention also provides methods of manipulating biological/chemical material. In one embodiment, the first and second droplets can be brought into proximity prior to coalescence by slowing or stopping at least one droplet comprising a first biological/chemical material by exerting a dielectrophoretic force onto the droplet produced by an electric field gradient. In another embodiment, the first and second droplets can be brought into proximity prior to coalescence where the first and second droplet are of different size. In some embodiments, one of the first and second droplets can be the size of the channel width and the other droplet can be smaller than the channel width. In other embodiments, the larger droplet has enough volume so that it would have a diameter greater than the channel width if it were spherical. In a further embodiment, the first and second droplets can be brought into proximity prior to coalescence where the first and second droplet are of different viscosities and thus move at different velocities. Viscosity of a droplet can be changed by changing the content of the droplet. For example, glycerol can be added to a droplet to give it an increased viscosity.

In one embodiment, the method of manipulating biological and chemical material, further comprises coalescing at least one droplet with a droplet slowed or stopped under the influence of a dielectrophoretic force from an electric field gradient created within a coalescence module, thereby producing a nanoreactor.

The droplet size can be controlled such that the droplet formed from flowing a first dispersed phase fluid in a continuous phase fluid moves at a different velocity with respect to a droplet formed from flowing a second dispersed phase fluid in a continuous phase fluid, such that droplets arrive in pairs at a region where an electric field induces them to coalesce, thereby producing a nanoreactor. In some embodiments, greater than 50% of the droplets are paired. In other embodiments, greater than 75% of the droplets are paired.

The droplet viscosity can be controlled such that the droplet formed from flowing a first dispersed phase fluid in

a continuous phase fluid moves at a different velocity with respect to the droplet formed from flowing a second dispersed phase fluid in a continuous phase fluid, such that droplets arrive in pairs at a region where an electric field induces them to coalesce, thereby producing a nanoreactor. In some embodiments, greater than 50% of the droplets are paired. In other embodiments, greater than 75% of the droplets are paired.

The electrodes comprising metal alloy components may either terminate at fluid channels or be isolated from fluid channels. The electrodes can be constructed by filling the appropriate channels with metal alloy. One way this can be accomplished is to use positive pressure injection of the metal alloy in a melted state, such as with a syringe, into the channels, and then cool the metal alloy to a solid form. Another example is to use negative pressure to suck the metal alloy in a melted state into the channels, and then cool the metal alloy to a solid form. This can be accomplished for example by use of capillary forces. Another method of construction can use any of the above mentioned embodiments, and then flush out the metal alloy in a melted state with another liquid to define the geometry of the metal alloy components. Another example is to use any of the above mentioned embodiments, and then use a localized cold probe to define a solid termination point for the metal alloy, and then cool the remaining metal alloy to a solid form. A further example is to use another material, such as microscopic solder spheres or UV curable conductive ink, to form a barrier between fluid and metal alloy channels, to define the geometry of the metal alloy components.

The device can include a combination of both integrated metal alloy components and a patterned electrically conductive layer. The patterned electrically conductive layer can have features patterned such that their boundaries are within a leak-proof seal. The device can have a patterned electrically conductive feature as one of two charging electrodes and one integrated metal alloy component as the other of two charging electrodes. Alternatively, the device can have metal alloy components as the two halves of a bowtie antenna and patterned electrically conductive features as the two halves of a pickup antenna for dielectric droplet detection.

The device can include a plurality of electrodes that are insulated from the fluid present in the device, and the method of operation including appropriate application of dielectrical signals and appropriate fluids. In known devices, the electrodes are typically in contact with the fluids in order to allow discharge of species that would otherwise screen the applied dielectric field. Whereas, in devices where the electrodes have been insulated from the fluid, this screening effect typically arises so quickly that the device is not useful for any significantly extended period of time. The drawbacks of electrodes in contact with the fluids vs. insulated electrodes are (a) degraded reliability against leaking (since the interface between the electrodes and the other components of the device may be more difficult to effect a leak-proof seal), and (b) degraded reliability against electrode corrosion (whose failure mode effects include failure of application of dielectric fields, and fluid channel contamination).

The device of the present invention comprising a plurality of electrodes that are insulated from the fluid present in the device counteracts this screening effect by extending the screening rise time and including a polarity switch for all of the different dielectric fields applied in the device. The screening rise time is extended by using fluids with dielectrical properties. A polarity switch for all of the different dielectric fields applied in the device is achieved by using an algorithm for dielectrical control, which switches the polar-

ity of the dielectrical fields at a frequency sufficiently high to maintain proper dielectrical function of the device. This dielectrical control algorithm may also switch the polarity for the dielectric fields in a cascading, time controlled manner starting at the fluid origin point and progressing downstream, so that given fluid components experience one polarity at every point along their course. The device of the present invention can be used with metal alloy electrodes or using a combination of metal alloy electrodes and patterned conductive film electrodes.

In one embodiment, the invention provides a microfluidic device using injected electrodes. The interface between the microscopic electrode (typically 25 μm thick) and the macroscopic interconnect can easily fail if the joint between the two is flexed. The flexing of the joint can be eliminated by securing a firm material that serves to fasten, support, and reinforce the joint (i.e., a grommet) into the interface. In order to prevent flexing, the mating surface of the device can be manufactured from a hard material such as glass or plastic. The electrical connection with the external system can be made by securing the device such that it connects to a spring loaded contact, which is either offset from the grommet (thereby minimizing the force applied to the solder region), or centered on the grommet (as long as the contact does not touch the solder).

The metal alloy components are also useful for performing optical functions on fluids, including but not limited to, optical detection of droplets in a geometry which may include a mirror.

To prevent leakage of fluid out of electrodes placed within microfluidic channels, the microfluidic device can include a layer patterned with channels for fluid control, and another layer with patterned electrically conductive features, where the features are patterned such that their boundaries are within a leak-proof seal. The leak-proof seal can be achieved at the interface between the unpatterned areas of the fluid control layer and the unpatterned areas of the electrically conductive layer. The leak-proof seal can also be achieved by a third interfacial layer between the fluid control layer and the unpatterned areas of the electrically conductive layer. The third interfacial layer can or can not be perforated at specific locations to allow contact between the fluid and the electrically conductive layer. Electrical access ports can also be patterned in the fluid control layer.

The electrodes and patterned electrically conductive layers as described can be associated with any module of the device (inlet module, coalescence module, mixing module, delay module, detection module and sorting module) to generate dielectric or electric fields to manipulate and control the droplets and their contents.

The microfluidic device can combine dielectric or electric fields with droplet fission to separate ionic species during droplet breakup.

The present invention provides methods of controlling droplets using fringing fields. Effective control of uncharged droplets within microfluidic devices can require the generation of extremely strong dielectric field gradients. The fringe fields from the edges of a parallel plate capacitor can provide an excellent topology to form these gradients. The microfluidic device according to the present invention can include placing a fluidic channel between two parallel electrodes, which can result in a steep electric field gradient at the entrance to the electrodes due to edge effects at the ends of the electrode pair. Placing these pairs of electrodes at a symmetric channel split can allow precise bi-directional control of droplet within a device. Using the same principle, only with asymmetric splits, can allow single ended control

of the droplet direction in the same manner. Alternatively, a variation on this geometry will allow precise control of the droplet phase by shifting.

A device of the invention can be used for the application of an electric field at a junction between two immiscible fluids. The electric field created charged droplets and large forces necessary for emulsification, while the junction stabilized droplet production even at high fields, when a Taylor cone was present. Applications of this technology include, but are not limited to, the generation of charged droplets with a narrow distribution in radius down to submicron sizes and controlled droplet coalescence by oppositely charged droplets.

The device of this embodiment can be created by patterning PDMS on a glass substrate having electrodes formed from indium tin oxide ("ITO"). A voltage difference can be applied to the electrodes to create an applied dielectric field. The device can include a two-fluid injection system where a conductive fluid can be injected into a non-conductive fluid in the presence of the electric field to generate droplets of the conductive fluid dispersed in the non-conductive fluid. Droplets can be created having diameters of less than about 1 micron to about 100 microns. These droplets can remain charged with the sign of the charge dependent on the sign of the dielectric field with respect to the direction of flow.

In the absence of an electric field, large droplets can be generated, while in the presence an electric field ($E=2$ V/micron), a Taylor cone can be stabilized with uniform submicron droplets being emitted from the tip. The droplets may also be discharged on a ground electrode located further downstream. Such a device can have many applications, for example, in generating well controlled nanoemulsions.

Oppositely oriented devices can also be used to generate droplets having opposite sign of charge. Using this charge, the droplets can coalesce at a precise or generally predetermined location. If there is no electric field applied, the droplets cannot coalesce. The electrostatic attraction can cause the drops to coalesce. The electric field, in some cases, can be used to control the phase between when the droplets are generated to ensure simultaneous arrival at a central location and subsequent coalescence, for example, through an auto feedback mechanism or a using an AC dither. The surface of the droplets can be deformed and electrostatic forces may overcome surface tension to produce a fluid bridge to coalesce and/or neutralize the droplets.

Interdigitation and Coalescence of Droplets

Particular design embodiments of the microfluidic device described herein allow for a more reproducible and controllable interdigitation of droplets of specific liquids followed by pair-wise coalescence of these droplets. The droplet pairs can contain liquids of different compositions and/or volumes, which would then combine to allow for a specific reaction to be investigated. The pair of droplets can come from any of the following: (i) two continuous aqueous streams and an oil stream; (ii) a continuous aqueous stream, an emulsion stream, and an oil stream, or (iii) two emulsion streams and an oil stream. FIG. 17 A-D.

The nozzle design enhances the interdigitation of droplets and further improves coalescence of droplets due to the better control of the interdigitation and smaller distance between pairs of droplets. The greater control over interdigitation allows for a perfect control over the frequency of either of the droplets. Coalescence can be accomplished by localized electric field application, as described above. Coalescence may also be accomplished by passive coalescence of droplets (i.e., without application of any external effects for the appropriate mix). Passive coalescence signifi-

cantly simplifies the device operation and control, which is critical as the same procedure is repeated multiple times in a given process. To obtain the optimum operation, the spacing between droplets and coupling of the droplets can be adjusted by adjusting flow of any of the streams, viscosity of the streams, nozzle design (including orifice diameter, the channel angle, and post-orifice neck of the nozzle).

In one embodiment, passive coalescence of paired droplets can be achieved by passing the droplets through a narrowing of a channel (or a neck-down or a pinch). FIG. 18A-D. In such an embodiment, droplets passing through the pinch are touching while being elongated as they are passing through the channel. Due to the elongation and redistribution of surface activities at the elongated ends, the droplet pair coalesces spontaneously and passively.

Detection Module

A "detection module" is a location within the device, typically within the main channel where molecules, cells, small molecules or particles are to be detected, identified, measured or interrogated on the basis of at least one predetermined characteristic. The molecules, cells, small molecules or particles can be examined one at a time, and the characteristic is detected or measured optically, for example, by testing for the presence or amount of a reporter. For example, the detection module is in communication with one or more detection apparatuses. The detection apparatuses can be optical or electrical detectors or combinations thereof. Examples of suitable detection apparatuses include optical waveguides, microscopes, diodes, light stimulating devices, (e.g., lasers), photo multiplier tubes, and processors (e.g., computers and software), and combinations thereof, which cooperate to detect a signal representative of a characteristic, marker, or reporter, and to determine and direct the measurement or the sorting action at the sorting module.

A detection module is within, communicating or coincident with a portion of the main channel at or downstream of the inlet module and, in sorting embodiments, at, proximate to, or upstream of, the sorting module or branch point. Precise boundaries for the detection module are not required, but are preferred. The sorting module may be located immediately downstream of the detection module or it may be separated by a suitable distance consistent with the size of the molecules, the channel dimensions and the detection system. It will be appreciated that the channels may have any suitable shape or cross-section (for example, tubular or grooved), and can be arranged in any suitable manner so long as flow can be directed from inlet to outlet and from one channel into another.

The detection module can have features to detect the droplets, including but not limited to, integrated metal alloy components and/or features patterned in an electrically conductive layer, to broadcast a signal around a droplet and pick up an electrical signal in proximity to the droplet.

As each droplet passes into the detection module, it is examined for a predetermined characteristic (i.e., using the detector) and a corresponding signal is produced, for example indicating that "yes" the characteristic is present, or "no" it is not. The signal may correspond to a characteristic qualitatively or quantitatively. That is, the amount of the signal can be measured and can correspond to the degree to which a characteristic is present. For example, the strength of the signal may indicate the size of a molecule, or the potency or amount of an enzyme expressed by a cell, or a positive or negative reaction such as binding or hybridization of one molecule to another, or a chemical reaction of a substrate catalyzed by an enzyme. In response to the signal, data can be collected and/or a control system in the sorting

module, if present, can be activated to divert a droplet into one branch channel or another for delivery to the collection module or waste module. Thus, in sorting embodiments, molecules or cells within a droplet at a sorting module can be sorted into an appropriate branch channel according to a signal produced by the corresponding examination at a detection module. The detection can be optical detection of molecular, cellular or other characteristics, for example directly or by use of a reporter associated with a characteristic chosen for sorting. However, other detection techniques can also be employed.

The device can be used to generate droplets whose composition may vary from one to the next due to any number of reasons (chemical reaction, sample preparation, etc). Within the same device, the droplets are passed through a measurement volume in which the contents are interrogated using various means (optical or electrical). The result of the measurement is used to decide which flow path the droplets should take. The means of changing the flow path can be accomplished through mechanical, electrical, optical, or some other technique as described herein.

The device can provide an accurate means of precisely aligning optical waveguides and their associated optical elements (lenses, prisms, mirrors, interconnects, etc.) to the fluidic channels contained within the microfluidic device. Such waveguides can be used to provide well defined optical access to the fluidic channels to permit optical scattering, absorption, fluorescence, or any other optical measurement technique.

Channels within the device are typically made using semiconductor lithographic processes. In order to create the waveguides, a separate series of channels and useful shapes (lenses, mirrors, etc) can be created either simultaneously (i.e. in the same processing step) or in successive steps. The reusable master created in this way can then be used to fabricate the waveguide components and fluid channels without the need for special fixturing or careful alignment in subsequent steps. The extra channels or shapes can then be filled with a high index of refraction liquid (for waveguides) or reflective material (for mirrors) through injection into the channel or void. The liquid can either remain as a fluid or be allowed to solidify. UV cure epoxies used by the telecommunications industry are excellent choices for the waveguide materials. Possible waveguide geometry can include a focusing lens and a back-reflecting mirror.

The device of the present invention also comprises the use of beads and methods for analyzing and sorting beads (i.e., bead reader device). The device can read and either sort or not sort droplets containing one or more of a set of two or more beads. Each bead can be differentiated from each other bead within a set. Beads can be separated by several tags including, but not limited to, quantum dyes, fluorescent dyes, ratios of fluorescent dyes, radioactivity, radio-tags, etc. For example, a set of beads containing a ratio of two dyes in discrete amounts with an apparatus for detecting and differentiating beads containing one discrete ratio from the other beads in this set having a different ratio of the two dyes. The microfluidic device can include a paramagnetic beads. The paramagnetic beads can introduce and remove chemical components from droplets using droplet coalescence and breakup events. The paramagnetic beads can also be used for sorting droplets.

The present invention provides methods of screening molecular libraries on beads through limited-delusion-loading and then chemical or optical release inside of droplets. Provided are methods for chemical synthesis on a bead and releasing said chemical attached to the bead using a releas-

ing means (chemical, UV light, heat, etc) within a droplet, and then combining a second droplet to the first droplet for further manipulation. For example, tea-bag synthesis of chemicals on a bead simultaneously with a means for identifying said bead (using, for example, a mass spec tag). Using the resulting mixed-chemistry beads in a droplet within a fluid flow, and exposing the beads to UV light to release the chemical synthesized from the bead into the droplet environment. Combining the droplet containing the released chemical with a droplet containing a cell, and performing a cell-based assay. Sorting droplets having the desired characteristics (for example, turn on of a reporter gene), and then analyzing the sorted beads using mass spectroscopy.

The device of the present invention can comprise column separation prior to bead sorting. A device containing a channel loaded with a separating means for chromatographically sorting the sample prior to droplet formation. Such separating means could include size, charge, hydrophobicity, atomic mass, etc. The separating can be done isocratic or by use of a means for generating a gradient chemically, (for example using salt or hydrophobicity), electrically, by pressure, or etc. For example, a channel is preloaded with Sepharose size exclusion media. A sample is loaded at one end, and the droplets are formed at an opposing end. The sample separates by size prior to becoming incorporated within a droplet.

The detector can be any device or method for interrogating a molecule, a cell or particle as it passes through the detection module. Typically, molecules, cells or particles (or droplets containing molecules, cells or particles) are to be analyzed or sorted according to a predetermined characteristic that is directly or indirectly detectable, and the detector is selected or adapted to detect that characteristic. A preferred detector is an optical detector, such as a microscope, which may be coupled with a computer and/or other image processing or enhancement devices to process images or information produced by the microscope using known techniques. For example, molecules can be analyzed and/or sorted by size or molecular weight. Enzymes can be analyzed and/or sorted by the extent to which they catalyze chemical reaction of a substrate (conversely, substrate can be analyzed and/or sorted by the level of chemical reactivity catalyzed by an enzyme). Cells can be sorted according to whether they contain or produce a particular protein, by using an optical detector to examine each cell for an optical indication of the presence or amount of that protein. The protein may itself be detectable, for example by a characteristic fluorescence, or it may be labeled or associated with a reporter that produces a detectable signal when the desired protein is present, or is present in at least a threshold amount. There is no limit to the kind or number of characteristics that can be identified or measured using the techniques of the invention, which include without limitation surface characteristics of the cell and intracellular characteristics, provided only that the characteristic or characteristics of interest for sorting can be sufficiently identified and detected or measured to distinguish cells having the desired characteristic(s) from those which do not. For example, any label or reporter as described herein can be used as the basis for analyzing and/or sorting molecules or cells, i.e. detecting molecules or cells to be collected.

The molecules or cells or particles (or droplets containing them) are analyzed and/or separated based on the intensity of a signal from an optically-detectable reporter bound to or associated with them as they pass through a detection module in the device. Molecules or cells or particles having

an amount or level of the reporter at a selected threshold or within a selected range are diverted into a predetermined outlet or branch channel of the device. The reporter signal may be collected by a microscope and measured by a photo multiplier tube (PMT). A computer digitizes the PMT signal and controls the flow via valve action or electro-osmotic potentials. Alternatively, the signal can be recorded or quantified as a measure of the reporter and/or its corresponding characteristic or marker, e.g., for the purpose of evaluation and without necessarily proceeding to sort the molecules or cells.

The chip can be mounted on an inverted optical microscope. Fluorescence produced by a reporter is excited using a laser beam focused on molecules (e.g., DNA, protein, enzyme or substrate) or cells passing through a detection region. Fluorescent reporters can include, but are not limited to, rhodamine, fluorescein, Texas red, Cy 3, Cy 5, phycobiliprotein (e.g., phycoerythrin), green fluorescent protein (GFP), YOYO-I and PicoGreen. In molecular fingerprinting applications, the reporter labels can be fluorescently labeled single nucleotides, such as fluorescein-dNTP, rhodamine-dNTP, Cy3-dNTP, etc.; where dNTP represents dATP, dTTP, dUTP or dCTP. The reporter can also be chemically-modified single nucleotides, such as biotin-dNTP. The reporter can be fluorescently or chemically labeled amino acids or antibodies (which bind to a particular antigen, or fragment thereof, when expressed or displayed by a cell or virus).

The device can analyze and/or sort cells based on the level of expression of selected cell markers, such as cell surface markers, which have a detectable reporter bound thereto, in a manner similar to that currently employed using fluorescence-activated cell sorting (SACS) machines. Proteins or other characteristics within a cell, and which do not necessarily appear on the cell surface, can also be identified and used as a basis for sorting. The device can also determine the size or molecular weight of molecules such as polynucleotides or polypeptides (including enzymes and other proteins) or fragments thereof passing through the detection module. Alternatively, the device can determine the presence or degree of some other characteristic indicated by a reporter. If desired, the cells, particles or molecules can be sorted based on this analysis. The sorted cells, particles or molecules can be collected from the outlet channels in collection modules (or discarded in wasted modules) and used as needed. The collected cells, particles or molecules can be removed from the device or reintroduced to the device for additional coalescence, analysis and sorting.

To detect a reporter or determine whether a molecule, cell or particle has a desired characteristic, the detection module may include an apparatus for stimulating a reporter for that characteristic to emit measurable light energy, e.g., a light source such as a laser, laser diode, light emitting diode (LED), high-intensity lamp, (e.g., mercury lamp), and the like. Where a lamp is used, the channels are preferably shielded from light in all regions except the detection module. Where a laser is used, the laser can be set to scan across a set of detection modules from different analysis units. In addition, laser diodes or LED's may be microfabricated into the same chip that contains the analysis units. Alternatively, laser diodes or LED's may be incorporated into a second chip (i.e., a laser diode chip) that is placed adjacent to the microfabricated analysis or sorter chip such that the laser light from the diodes shines on the detection module(s).

An integrated semiconductor laser and/or an integrated photodiode detector can be included on the silicon wafer in the vicinity of the detection module. This design provides

the advantages of compactness and a shorter optical path for exciting and/or emitted radiation, thus minimizing distortion and losses.

The present invention provides methods of droplet detection using electrical signal broadcasting. The device of the present invention can comprise features, such as integrated metal alloy components and/or features patterned in an electrically conductive layer, for detecting droplets by broadcasting a signal around a droplet and picking up an electrical signal in proximity to the droplet.

The present invention provides self-aligning optical waveguides and optical elements for detection and control of droplets. The device of the present invention can comprise an accurate means of precisely aligning optical waveguides and their associated optical elements (lenses, prisms, mirrors, interconnects, etc.) to the fluidic channels contained within the device. Such waveguides can be used to provide well defined optical access to the fluidic channels to permit optical scattering, absorption, fluorescence, or any other optical measurement technique.

Fluidic channels within a microfluidic device are typically made using semiconductor lithographic processes. In order to create the waveguides, a separate series of channels and useful shapes (lenses, mirrors, etc) can be created either simultaneously (i.e. in the same processing step) or in successive steps. The reusable master created in this way can then be used to fabricate the waveguide components and fluid channels without the need for special fixturing or careful alignment in subsequent steps. The extra channels or shapes can then be filled with a high index of refraction liquid (for waveguides) or reflective material (for mirrors) through injection into the channel or void. The liquid can either remain as a fluid or be allowed to solidify. UV cure epoxies used by the telecommunications industry are excellent choices for the waveguide materials. Possible waveguide geometries can include a focusing lens and a back-reflecting mirror.

The dimensions of the detection module are influenced by the nature of the sample under study and, in particular, by the size of the droplets, beads, particles, molecules or cells (including virions) under study. For example, mammalian cells can have a diameter of about 1 to 50 microns, more typically 10 to 30 microns, although some mammalian cells (e.g., fat cells) can be larger than 120 microns. Plant cells are generally 10 to 100 microns. However, other molecules or particles can be smaller with a diameter from about 20 nm to about 500 nm.

Detection modules used for detecting molecules and cells have a cross-sectional area large enough to allow a desired molecule, cells, bead, or particles to pass through without being substantially slowed down relative to the flow carrying it.

In another embodiment, the droplet content detection can be achieved by simultaneous detection of contents of multiple droplets in parallel using spectroscopic fluorescence imaging with sensitivity as high as single-molecule limit. In this embodiment, one can spatially distribute droplets containing fluorescent entities such as Fluorophore biological markers and/or quantum dots in a two-dimensional sheet in a microscopic field-of-view. The field-of-view of those droplets can then be illuminated by a fluorescence excitation source and the resulting fluorescence can be spectroscopically imaged. Therefore, for a given fluorescence detection sensitivity, the throughput of fluorescence detection compared to a single-drop fluorescence detection method can be increased by a factor of a/b for a given sensitivity, where a is the number of droplets that can be imaged within a given

field-of-view, and b is the ratio of the fluorescence sensitivity of a single-drop fluorescence detector compared to that of the multiple drop fluorescence detector. Furthermore, unlike the prior art single-drop fluorescent detection method where the drops are flowed through a detection volume so that their residence time in the detection volume, and hence the signal integration time and sensitivity, is limited, the residence time of the droplet in the field-of-view can be unlimited, thereby allowing sensitivity as high as the single-molecule limit.

Sorting Module

The device of the present invention can further include one or more sorting modules. A "sorting module" is a junction of a channel where the flow of molecules, cells, small molecules or particles can change direction to enter one or more other channels, e.g., a branch channel for delivery to an outlet module (i.e., collection or waste module), depending on a signal received in connection with an examination in the detection module. Typically, a sorting module is monitored and/or under the control of a detection module, and therefore a sorting module may "correspond" to such detection module. The sorting region is in communication with and is influenced by one or more sorting apparatuses. A sorting apparatus comprises techniques or control systems, e.g., dielectric, electric, electro-osmotic, (micro-) valve, etc. A control system can employ a variety of sorting techniques to change or direct the flow of molecules, cells, small molecules or particles into a predetermined branch channel. A "branch channel" is a channel which is in communication with a sorting region and a main channel. Typically, a branch channel receives molecules, cells, small molecules or particles depending on the molecule, cells, small molecules or particles characteristic of interest as detected by the detection module and sorted at the sorting module. A branch channel can have an outlet module and/or terminate with a well or reservoir to allow collection or disposal (collection module or waste module, respectively) of the molecules, cells, small molecules or particles. Alternatively, a branch channel may be in communication with other channels to permit additional sorting.

The device of the present invention can further include one or more outlet modules. An "outlet module" is an area of a microfabricated device that collects or dispenses molecules, cells, small molecules or particles after coalescence, detection and/or sorting. The outlet module can include a collection module and/or a waste module. The collection module can be connected to a means for storing a sample. The collection module can be a well or reservoir for collecting and containing droplets detected to have a specific predetermined characteristic in the detection module. The collection module can be temperature controlled. The waste module can be connected to a means for discarding a sample. The waste module can be a well or reservoir for collecting and containing droplets detected to not have a specific predetermined characteristic in the detection module. The outlet module is downstream from a sorting module, if present, or downstream from the detection module if a sorting module is not present. The outlet module may contain branch channels or outlet channels for connection to a collection module or waste module. A device can contain more than one outlet module.

Mixing Module

Although coalescence of one or more droplets in one or more coalescence modules can be sufficient to mix the contents of the coalesced droplets (e.g., through rotating vortexes existing within the droplet), the device of the present invention can further include one or more mixing modules. A "mixing module" can comprise features for

shaking or otherwise manipulate droplets so as to mix their contents. The mixing module is preferably downstream from the coalescing module and upstream from the detection module. The mixing module can include, but is not limited to, the use of metal alloy component electrodes or electrically conductive patterned electrodes to mix the contents of droplets and to reduce mixing times for fluids combined into a single droplet in the microfluidic device.

The device of the present invention can comprise features, such as, acoustic actuators, metal alloy component electrodes or electrically conductive patterned electrodes, for shaking droplets to reduce mixing times for fluids combined into a single droplet.

For acoustic manipulation, the frequency of the acoustic wave should be fine tuned so as not to cause any damage to the cells. The biological effects of acoustic mixing have been well studied (e.g., in the ink-jet industry) and many published literatures also showed that piezoelectric microfluidic device can deliver intact biological payloads such as live microorganisms and DNA. In an exemplary embodiment, the design of the acoustic resonant uses a Piezoelectric bimorph flat plate located on the side of the carved resonant in the PDMS slab. The piezoelectric driving waveform is carefully optimized to select the critical frequencies that can separate cells in fluids. There are five parameters to optimize beyond the frequency parameter. Lab electronics is used to optimize the piezoelectric driving waveform. Afterwards, a low cost circuit can be designed to generate only the optimized waveform in a preferred microfluidic device.

Delay Module

The device of the present invention can further include one or more delay modules. The "delay module" can be a delay line. The operation of a microfluidics device where a reaction within a droplet is allowed to occur for a non-trivial length of time requires a delay line to increase the residence time within the device. For reactions demanding extensive residence time, longer or larger delay lines are required. Accordingly, the invention provides methods to increase residence times within microfluidic devices.

The delay module is in fluid communication with the main channel. The delay module can be located downstream of the coalescence module and upstream of the detection module. The delay module can be a serpentine channel or a buoyant hourglass. The delay module can further comprise heating and cooling regions. The heating and cooling regions can be used for performing on-chip, flow-through PCR with the devices described herein.

The channel dimensions and configurations can be designed to accommodate the required residence time with minimum pressure drops across the device. For example, to accommodate very long delay lines within the microfluidic device, the device can comprise a multilayered PDMS slab which is composed of several patterned PDMS slabs.

The channel dimensions can also be designed so as to allow for required flow, residence time and pressure drop. Some channels may be required to be very large in width and height. In order to avoid collapse of the channels, the device includes support posts within the channel design. In order to reduce dead volume behind posts and further improve droplet stability, the support posts are designed to optimize a streamlined flow within the channel. These designs can include curved features as opposed to sharp edges.

To allow for longer period of device operation, delay lines can also be extended to the outside of the chip. The off-chip delay lines can be tubes within micron-sized internal diameter.

In order to allow more efficient use of available space and faster operation, in methods where droplets are charged, after charging, asymmetric splitting of oil and drops can be accommodated by siphoning off oil from channels after droplets are charged. The delay lines can be in the form of a tower (i.e., a structure which is vertical with respect to the ambient gravitational field) as to allow buoyant forces to assist controlled droplet transport. Known delay lines involve transporting droplets by emulsifying them in a carrier fluid flowing in a channel and/or tube. Because the velocity profile of the carrier fluid through the cross-section of the channel and/or tube is not uniform, the velocity distribution of the droplets will not be narrow, which causes the delay time distribution of the droplets to not be narrow (i.e., some droplets will be delayed more or less than others).

The devices of the present invention can also include buoyancy-assisted microfluidic delay lines. In buoyancy-assisted microfluidic delay lines, buoyant forces act on droplets emulsified in a fluid in one or more towers. This can include allowing the tower to fill for the desired delay time, and then releasing the droplets. The tower can or cannot continue to fill and release droplets as needed. In this example, one may desire to have a cylindrical tower section that is capped by a pyramidal funnel section. The tower can effectively function as an hourglass. Droplets that have a density less than their carrier fluid are fed into the base of the tower, buoyantly rise to the top of the tower with a substantially uniform velocity distribution, and are funneled into a functional component of the microfluidic device (such as a y-branch). Carrier fluid is exhausted at the base of the tower at the same rate as it is introduced at the apex so that the net flow of carrier fluid through the delay line is zero. The tower and funnel sections can have any cross-sectional shape, such as circular, elliptical, or polygonal. The microfluidic device can include a tower with adjustable length.

The device can also include a switching network of twenty towers to guarantee a delay time dispersion of 5% (because $1/20=0.05$). The capacity of each tower is $0.05 \cdot T$, where T is the delay time. The concept includes, for example: (a) upon device start-up, filling the first tower for $0.05 \cdot T$, but stop-cock its exhaust, and also have the other nineteen towers closed; (b) after $0.05 \cdot T$, closing the first tower and filling the second between $0.05 \cdot T$ and $0.10 \cdot T$; (c) repeating step (b) for the remaining eighteen towers; (d) at time T , allowing the first tower to exhaust; (e) at time $1.05 \cdot T$, stop-cocking the exhaust of the first tower, allowing the second tower to exhaust, and allowing the first tower to fill; (f) at time $1.10 \cdot T$, stop-cocking the exhaust of the second tower, allowing the third tower to exhaust, closing the first tower, and allowing the second tower to fill, and (g) repeating step (f) ad infinitum. More than twenty towers may provide an even tighter control over the width of the delay time dispersion. This scheme may require a valve network. This network of towers can be outside the microfluidic device.

UV-Release Module

The device of the present invention can further include one or more UV-release modules. The "UV-release module" is in fluid communication with the main channel. The UV-release module is located downstream of the inlet module and upstream of the coalescence module. The UV-module can be used in bead assays. Compounds from encapsulated beads can be cleaved in a UV-releasing module using UV light. Photolabile linkers can be broken down on demand after a single bead has been encapsulated thus releasing multiple copies of a single compound into solution. In the cell based assay disclosed herein the chemical

compound assayed is desired to be in solution in order to penetrate the cell membrane. Furthermore, to ensure compartmentalization of a single compound with a cell the cleavage of the compound from the solid support can only be done after the bead has been encapsulated. Photocleavable linkers can be utilized to cleave the compounds of the bead after drop formation by passing the drop through a UV-release module (i.e., laser of the appropriate wavelength).

The present invention also provides methods for chemical synthesis on a bead and releasing said chemical attached to the bead using a releasing means (chemical, UV light, heat, etc) within a droplet, and then combining a second droplet to the first droplet for further manipulation. Preferably, the releasing means is a UV-module. For example, tea-bag synthesis of chemicals on a bead simultaneously with a means for identifying said bead (using, for example, a mass spec tag). Using the resulting mixed-chemistry beads in a droplet within a fluid flow, and exposing the beads to UV light to release the chemical synthesized from the bead into the droplet environment. Combining the droplet containing the released chemical with a droplet containing a cell, and performing a cell-based assay. Sorting droplets having the desired characteristics (for example, turn on of a reporter gene), and then analyzing the sorted beads using mass spectroscopy.

Kits

As a matter of convenience, predetermined amounts of the reagents, compound libraries, and/or emulsions described herein and employed in the present invention can be optionally provided in a kit in packaged combination to facilitate the application of the various assays and methods described herein. Such kits also typically include instructions for carrying out the subject assay, and may optionally include the fluid receptacle, e.g., the cuvette, multiwell plate, microfluidic device, etc. in which the reaction is to be carried out.

Typically, reagents included within the kit are uniquely labeled emulsions containing tissues, cells, particles, proteins, antibodies, amino acids, nucleotides, small molecules, substrates, and/or pharmaceuticals. These reagents may be provided in pre-measured container (e.g., vials or ampoules) which are co-packaged in a single box, pouch or the like that is ready for use. The container holding the reagents can be configured so as to readily attach to the fluid receptacle of the device in which the reaction is to be carried out (e.g., the inlet module of the microfluidic device as described herein). In one embodiment, the kit can include an RNAi kit. In another embodiment, the kit can include a chemical synthesis kit. It will be appreciated by persons of ordinary skill in the art that these embodiments are merely illustrative and that other kits are also within the scope of the present invention.

DEFINITIONS

The terms used in this specification generally have their ordinary meanings in the art, within the context of this invention and in the specific context where each term is used. Certain terms are discussed below, or elsewhere in the specification, to provide additional guidance to the practitioner in describing the devices and methods of the invention and how to make and use them. It will be appreciated that the same thing can typically be described in more than one way. Consequently, alternative language and synonyms may be used for any one or more of the terms discussed herein.

Synonyms for certain terms are provided. However, a recital of one or more synonyms does not exclude the use of other synonyms, nor is any special significance to be placed upon whether or not a term is elaborated or discussed herein. AU publications, patent applications, patents, and other refer-
 5 ences mentioned herein are incorporated by reference. In the case of conflict, the present specification, including defini- tions, will control. In addition, the materials, methods, and examples are illustrative only and are not intended to be limiting.

The invention is also described by means of particular examples. However, the use of such examples anywhere in the specification, including examples of any terms discussed herein, is illustrative only and in no way limits the scope and meaning of the invention or of any exemplified term. Like-
 10 wise, the invention is not limited to any particular preferred embodiments described herein. Indeed, many modifications and variations of the invention will be apparent to those skilled in the art upon reading this specification and can be made without departing from its spirit and scope. The invention is therefore to be limited only by the terms of the appended claims along with the full scope of equivalents to which the claims are entitled.

As used herein, “about” or “approximately” shall gener-
 25 ally mean within 20 percent, preferably within 10 percent, and more preferably within 5 percent of a given value or range.

The term “molecule” means any distinct or distinguish-
 30 able structural unit of matter comprising one or more atoms, and includes for example polypeptides and polynucleotides.

The term “polymer” means any substance or compound that is composed of two or more building blocks (‘mers’) that are repetitively linked to each other. For example, a “dimer” is a compound in which two building blocks have been joined together.

The term “polynucleotide” as used herein refers to a polymeric molecule having a backbone that supports bases capable of hydrogen bonding to typical polynucleotides, where the polymer backbone presents the bases in a manner to permit such hydrogen bonding in a sequence specific
 40 fashion between the polymeric molecule and a typical polynucleotide (e.g., single-stranded DNA). Such bases are typically inosine, adenosine, guanosine, cytosine, uracil and thymidine. Polymeric molecules include double and single stranded KNA and DNA, and backbone modifications thereof, for example, methylphosphonate linkages.

Thus, a “polynucleotide” or “nucleotide sequence” is a series of nucleotide bases (also called “nucleotides”) gener-
 45 ally in DNA and RNA, and means any chain of two or more nucleotides. A nucleotide sequence typically carries genetic information, including the information used by cellular machinery to make proteins and enzymes. These terms include double or single stranded genomic and cDNA, RNA, any synthetic and genetically manipulated polynucleotide, and both sense and anti-sense polynucleotide (al-
 50 though only sense stands are being represented herein). This includes single- and double-stranded molecules, i.e., DNA-DNA, DNA-RNA and RNA-RNA hybrids, as well as “protein nucleic acids” (PNA) formed by conjugating bases to an amino acid backbone. This also includes nucleic acids containing modified bases, for example thio-uracil, thio-
 55 guanine and fluoro-uracil.

The polynucleotides herein may be flanked by natural regulatory sequences, or may be associated with heterologous sequences, including promoters, enhancers, response
 60 elements, signal sequences, polyadenylation sequences, introns, 5'- and 3'-non-coding regions, and the like. The

nucleic acids may also be modified by many means known in the art. Non-limiting examples of such modifications include methylation, “caps”, substitution of one or more of the naturally occurring nucleotides with an analog, and
 5 internucleotide modifications such as, for example, those with uncharged linkages (e.g., methyl phosphonates, phosphotriesters, phosphoramidates, carbamates, etc.) and with charged linkages (e.g., phosphorothioates, phosphorodithio-
 10 ates, etc.). Polynucleotides may contain one or more additional covalently linked moieties, such as, for example, proteins (e.g., nucleases, toxins, antibodies, signal peptides, poly-L-lysine, etc.), intercalators (e.g., acridine, psoralen, etc.), chelators (e.g., metals, radioactive metals, iron, oxi-
 15 dative metals, etc.), and alkylators. The polynucleotides may be derivatized by formation of a methyl or ethyl phosphotriester or an alkyl phosphoramidate linkage. Furthermore, the polynucleotides herein may also be modified with a label capable of providing a detectable signal, either directly or indirectly. Exemplary labels include radioisotopes, fluores-
 20 cent molecules, biotin, and the like.

The term “interdigitation” as used herein means pairing of droplets from separate aqueous streams, or from two separate inlet nozzles, for eventual coalescence.

The term “dielectrophoretic force gradient” means a dielectrophoretic force is exerted on an object in an electric field provided that the object has a different dielectric constant than the surrounding media. This force can either pull the object into the region of larger field or push it out of the region of larger field. The force is attractive or repulsive depending respectively on whether the object or the surrounding media has the larger dielectric constant.

“DNA” (deoxyribonucleic acid) means any chain or sequence of the chemical building blocks adenine (A),
 35 guanine (G), cytosine (C) and thymine (T), called nucleotide bases, that are linked together on a deoxyribose sugar backbone. DNA can have one strand of nucleotide bases, or two complimentary strands which may form a double helix structure. “RNA” (ribonucleic acid) means any chain or sequence of the chemical building blocks adenine (A),
 40 guanine (G), cytosine (C) and uracil (U), called nucleotide bases, that are linked together on a ribose sugar backbone. RNA typically has one strand of nucleotide bases.

A “polypeptide” (one or more peptides) is a chain of chemical building blocks called amino acids that are linked together by chemical bonds called peptide bonds. A “pro-
 45 tein” is a polypeptide produced by a living organism. A protein or polypeptide may be “native” or “wild-type”, meaning that it occurs in nature; or it may be a “mutant”, “variant” or “modified”, meaning that it has been made, altered, derived, or is in some way different or changed from a native protein, or from another mutant.

An “enzyme” is a polypeptide molecule, usually a protein produced by a living organism, that catalyzes chemical reactions of other substances. The enzyme is not itself
 50 altered or destroyed upon completion of the reaction, and can therefore be used repeatedly to catalyze reactions. A “substrate” refers to any substance upon which an enzyme acts.

As used herein, “particles” means any substance that may be encapsulated within a droplet for analysis, reaction,
 60 sorting, or any operation according to the invention. Particles are not only objects such as microscopic beads (e.g., chromatographic and fluorescent beads), latex, glass, silica or paramagnetic beads, but also includes other encapsulating porous and/or biomaterials such as liposomes, vesicles and other emulsions. Beads ranging in size from 0.1 micron to 1 mm can be used in the devices and methods of the invention

and are therefore encompassed with the term “particle” as used herein. The term particle also encompasses biological cells, as well as beads and other microscopic objects of similar size (e.g., from about 0.1 to 120 microns, and typically from about 1 to 50 microns) or smaller (e.g., from about 0.1 to 150 nm). The devices and methods of the invention are also directed to sorting and/or analyzing molecules of any kind, including polynucleotides, polypeptides and proteins (including enzymes) and their substrates and small molecules (organic or inorganic). Thus, the term particle further encompasses these materials.

The particles (including, e.g., cells and molecules) are sorted and/or analyzed by encapsulating the particles into individual droplets (e.g., droplets of aqueous solution in oil), and these droplets are then sorted, combined and/or analyzed in a microfabricated device. Accordingly, the term “droplet” generally includes anything that is or can be contained within a droplet.

A “small molecule” as used herein, is meant to refer to a composition that has a molecular weight of less than about 5 kD and most preferably less than about 4 kD. Small molecules can be, e.g., nucleic acids, peptides, polypeptides, peptidomimetics, carbohydrates, lipids or other organic or inorganic molecules. Libraries of chemical and/or biological mixtures, such as fungal, bacterial, or algal extracts, are known in the art.

As used herein, “cell” means any cell or cells, as well as viruses or any other particles having a microscopic size, e.g. a size that is similar to or smaller than that of a biological cell, and includes any prokaryotic or eukaryotic cell, e.g., bacteria, fungi, plant and animal cells. Cells are typically spherical, but can also be elongated, flattened, deformable and asymmetrical, i.e., non-spherical. The size or diameter of a cell typically ranges from about 0.1 to 120 microns, and typically is from about 1 to 50 microns. A cell may be living or dead. Since the microfabricated device of the invention is directed to sorting materials having a size similar to a biological cell (e.g. about 0.1 to 120 microns) or smaller (e.g., about 0.1 to 150 nm) any material having a size similar to or smaller than a biological cell can be characterized and sorted using the microfabricated device of the invention. Thus, the term cell shall further include microscopic beads (such as chromatographic and fluorescent beads), liposomes, emulsions, or any other encapsulating biomaterials and porous materials. Non-limiting examples include latex, glass, or paramagnetic beads; and vesicles such as emulsions and liposomes, and other porous materials such as silica beads. Beads ranging in size from 0.1 micron to 1 mm can also be used, for example in sorting a library of compounds produced by combinatorial chemistry. As used herein, a cell may be charged or uncharged. For example, charged beads may be used to facilitate flow or detection, or as a reporter. Biological cells, living or dead, may be charged for example by using a surfactant, such as SDS (sodium dodecyl sulfate). The term cell further encompasses “virions”, whether or not virions are expressly mentioned.

A “virion”, “virus particle” is the complete particle of a virus. Viruses typically comprise a nucleic acid core (comprising DNA or RNA) and, in certain viruses, a protein coat or “capsid”. Certain viruses may have an outer protein covering called an “envelope”. A virion may be either living (i.e., “viable”) or dead (i.e., “non-viable”). A living or “viable” virus is one capable of infecting a living cell. Viruses are generally smaller than biological cells and typically range in size from about 20-25 nm diameter or less (parvoviridae, picornoviridae) to approximately 200-450 nm (poxyviridae). However, some filamentous viruses may reach

lengths of 2000 nm (closterviruses) and are therefore larger than some bacterial cells. Since the microfabricated device of the invention is particularly suited for sorting materials having a size similar to a virus (i.e., about 0.1 to 150 nm), any material having a size similar to a virion can be characterized and sorted using the microfabricated device of the invention. Non-limiting examples include latex, glass or paramagnetic beads; vesicles such as emulsions and liposomes; and other porous materials such as silica beads. Beads ranging in size from 0.1 to 150 nm can also be used, for example, in sorting a library of compounds produced by combinatorial chemistry. As used herein, a virion may be charged or uncharged. For example, charged beads may be used to facilitate flow or detection, or as a reporter. Biological viruses, whether viable or non-viable, may be charged, for example, by using a surfactant, such as SDS.

A “reporter” is any molecule, or a portion thereof, that is detectable, or measurable, for example, by optical detection. In addition, the reporter associates with a molecule, cell or virion or with a particular marker or characteristic of the molecule, cell or virion, or is itself detectable to permit identification of the molecule, cell or virion’s, or the presence or absence of a characteristic of the molecule, cell or virion. In the case of molecules such as polynucleotides such characteristics include size, molecular weight, the presence or absence of particular constituents or moieties (such as particular nucleotide sequences or restrictions sites). In the case of cells, characteristics which may be marked by a reporter includes antibodies, proteins and sugar moieties, receptors, polynucleotides, and fragments thereof. The term “label” can be used interchangeably with “reporter”. The reporter is typically a dye, fluorescent, ultraviolet, or chemiluminescent agent, chromophore, or radio-label, any of which may be detected with or without some kind of stimulatory event, e.g., fluoresce with or without a reagent. In one embodiment, the reporter is a protein that is optically detectable without a device, e.g. a laser, to stimulate the reporter, such as horseradish peroxidase (HRP). A protein reporter can be expressed in the cell that is to be detected, and such expression may be indicative of the presence of the protein or it can indicate the presence of another protein that may or may not be coexpressed with the reporter. A reporter may also include any substance on or in a cell that causes a detectable reaction, for example by acting as a starting material, reactant or a catalyst for a reaction which produces a detectable product. Cells may be sorted, for example, based on the presence of the substance, or on the ability of the cell to produce the detectable product when the reporter substance is provided.

A “marker” is a characteristic of a molecule, cell or virion that is detectable or is made detectable by a reporter, or which may be coexpressed with a reporter. For molecules, a marker can be particular constituents or moieties, such as restrictions sites or particular nucleic acid sequences in the case of polynucleotides. For cells and virions, characteristics may include a protein, including enzyme, receptor and ligand proteins, saccharrides, polynucleotides, and combinations thereof, or any biological material associated with a cell or virion. The product of an enzymatic reaction may also be used as a marker. The marker may be directly or indirectly associated with the reporter or can itself be a reporter. Thus, a marker is generally a distinguishing feature of a molecule, cell or virion, and a reporter is generally an agent which directly or indirectly identifies or permits measurement of a marker. These terms may, however, be used interchangeably.

The invention is further described below, by way of the following examples. The examples include descriptions of particular, exemplary embodiments of the devices and methods of the present invention, including particular embodiments of channel architectures, valves, switching and flow control devices and methods which may be implemented as part of the devices and methods of the invention. The examples are provided, for illustrative purposes only and are not limiting of the above-described invention in any way. For example, many of these specific embodiments are described and discussed primarily in terms of detecting and sorting cells suspended directly in the fluid that flows through a main channel of the device. Nevertheless, it will be appreciated by persons of ordinary skill in the art that these preferred embodiments are merely illustrative and that the invention may be practiced in a variety of embodiments that share the same inventive concept. In particular, the devices and methods described in this example (including the channel architectures, valves, switching and flow control devices and methods) may be readily adapted to a multiphased device so that droplets which contain, e.g., molecules, cells or virions may be analyzed and/or sorted as desired by a user.

EXAMPLES

Example 1

The device of the present invention can be used for Live/Dead Cell Based Assays. In one example, the assay uses two fluorophores; one is permeable across cell membranes, and a second dye binds DNA and can enter the cell only if the membrane is compromised. Similar Live/Dead assays exist for bacteria and yeast. Tagged chemical libraries and photocleavable linkers can be used in such assays. Combinatorial one-bead-one-compound libraries obtained through split-bead synthesis require a tag which describes their synthetic history in order to identify the compound reliably. Several encoding technologies for microcarriers such as beads, rods and crowns have been developed over the last decade to address this need. A simple and effective method relies on spectrometric chemical tags which are generated in parallel to the chemical entity of interested utilizing orthogonal chemistry. Alternatives include the use of nucleic acids such as DNA, followed by the use of the polymerase chain reaction (PCR) to decode the encoded beads.

In the cell based assay disclosed herein the chemical compound assayed is desired to be in solution in order to penetrate the cell membrane. Furthermore, to ensure compartmentalization of a single compound with a cell the cleavage of the compound from the solid support can only be done after the bead has been encapsulated. Photocleavable linkers can be utilized to cleave the compounds of the bead after drop formation by passing the drop through a UV-release module (i.e., laser of the appropriate wavelength).

To evaluate the effect of individual components contained in the molecular library, a two color fluorescence detection for standard cytotoxicity assays can be used [available from Invitrogen (Carlsbad, Calif.) or Cell Technology]. While any cells can be used, for illustrative purposes, the Invitrogen LIVE/DEAD Viability/Cytotoxicity Kit #L3224 for animal cells are used here. This kit contains two probes that measure two recognized parameters of cell viability: intracellular esterase activity and plasma membrane integrity. Live cells are identified by the presence of intracellular esterase activ-

ity, detected by the enzymatic conversion of the almost nonfluorescent cell-permeant calcein AM to the extremely fluorescent calcein. The calcein is retained within live cells, producing an intense uniform green fluorescence. EthD-1 enters cells with damaged membranes and undergoes a 40-fold enhancement of fluorescence upon binding to nucleic acids, thereby producing a bright red fluorescence in dead cells. EthD-1 is excluded by the intact plasma membrane of live cells. The determination of cell viability depends on these physical and biochemical properties of cells. Background fluorescence levels are inherently low with this assay technique because the dyes are essentially non-fluorescent before interacting with cells.

The spectral absorption and emission characteristics for both the calcein and EthD-1 are presented in FIG. 3, while FIG. 2 plots results presented by Molecular probes when a 50/50 mix of live and dead cells are run through a flow cytometer. The absorption characteristics of both dyes makes it possible to excite fluorescence using the existing 488 nm excitation source. FIG. 2, left panel, shows a mixture of live and ethanol-killed bovine pulmonary artery epithelial cells stained with the reagents in Molecular Probes Live/Dead Cell Viability/Cytotoxicity Assay Kit (L3224). Live cells fluoresce bright green, whereas dead cells with compromised membranes fluoresce red-orange. (Molecular Probes). The middle panel shows a viability assay using Molecular Probes' LIVE/DEAD Viability/Cytotoxicity Kit on a flow cytometer. A 1:1 mixture of live and ethanol-fixed human B cells was stained with calcein AM and ethidium homodimer-1, flow cytometric analysis was carried out with excitation at 488 nm. The right panel shows analysis of bacterial cultures using the Live/Dead BacLight Bacterial Viability and Counting Kit available from www.molecularprobes.com. As shown in FIG. 3, left panel, the present invention further provides a fluorescence detection system comprising a fluorescence detection stand capable of measuring green fluorophores within microfluidic channels while simultaneously permitting visual monitoring via a high speed video microscope. The optical components of this system are commercially available. The modular layout of this system permits straightforward modification of the excitation and detection wavelengths. This modularity also makes it possible to upgrade the system to multi-wavelength excitation, multi wavelength detection, and detection of orthogonal polarization states. Currently, the 488 nm transition of a multiline Argon-Ion Laser is used as the excitation source for Fluorescein (FITC). The laser provides between 3 and 20 milliwatts of power and is focused to a spot approximately 17 microns in diameter (full width half maximum, FWHM). When the stand is configured to use a photomultiplier tube, it is able to detect less than 10,000 FITC molecules at a 10 kHz droplet rate. The sensitivity of this system is limited by fluorescence interference generated by the microfluidic device itself. The right panel of FIG. 3 shows excitation and emission spectra for calcein AM and EthD-1 dyes. Normal cytometry protocol excites both at 488 nm. FIG. 3 indicated the changes required to convert the single fluorophore station to a two color fluorescence station. The calcein fluorescence can be collected using filters designed for fluorescein detection, while the EthD-1 can be monitored using filters designed for propidium iodide or Texas Red.

Using water droplets doped with fluorescein and propidium iodide over a range of concentrations from 1×10^{-3} M to 1×10^{-8} M, both dyes have similar absorption and fluorescence properties to calcein and Ethd-1. In seventeen micron droplets, this corresponds to a range of 1.5×10^9 to

1.5×10⁴ molecules within the measurement volume. Once the baseline performance has been verified, tests can begin on droplets containing live cells, dead cells, and mixtures of the two. This establishes selectivity and detection limits on the two types of cells.

The dyes selected have been used extensively in flow cytometry and are commonly used in most cell-based assays. They are designed not to overlap significantly with each other and can be evaluated both independently and together to assess the cross-talk. The status of (potentially) many cells within one drop can thus be determined. The use of inexpensive optics on our instrument will be more than compensated for by the theoretical increase of dye molecules in the nanoreactor. Optics with higher efficiencies can be used.

Compounds from encapsulated beads can be cleaved in a UV-releasing module using UV light. Photolabile linkers can be broken down on demand after a single bead has been encapsulated thus releasing multiple copies of a single compound into solution.

Synthetic chemistry relies on the differential activity of chemical groups in order to control bond breaking and forming processes. Photolabile protecting groups form a fourth orthogonal type of functionality which survive reaction conditions capable of cleaving protective groups of the other types. Several of these photolabile protecting groups have been used to link organic molecules to solid support and their use as linkers has been reviewed. This allows the synthesis of solid supported molecules with the option of releasing the final product by irradiation with the appropriate wavelength. The repertoire of chemical groups for which photocleavable protecting groups have been devised is extensive, which allows the synthesis of diverse combinatorial libraries.

In lieu of the high sample rate a triazene-based photolabile linker, which is cleaved by irradiation with a 355 nm 3w Nd-YAG laser, can be used. This linker is stable under a wide range of reaction conditions with the exception of strong acids lending itself to solid supported split-bead synthesis.

If the residence time of the bead inside the UV laser is insufficient to cleave all of the compound off the substrate bead, the residence time can be increased by slowing down the flow of the bead containing drops by widening the channel. Alternatively the intensity of laser beam can be increased to ensure complete cleavage.

As previously discussed, long incubation times are desirable for cytotoxicity studies, but cannot be easily achieved in known microfluidic channel layouts. Accordingly, one embodiment of the device used in the live/dead cell-based assay disclosed herein uses a passive means to achieve uniform droplet residency times exceeding one hour in a delay line module located directly before the sorting module. It is possible to achieve a delay time of one hour between droplet generation and detection without stopping droplet generation.

In one example, a “buoyancy hourglass” delay line can be used, wherein, similar to sands in an hourglass which depend on gravity, the droplets will rise from a large reservoir to an exhaust port due to their density mismatch with the carrier oil. Microfluidic modules (e.g., inlet module, UV-releasing module, coalescence module, and mixing module) which are utilized before the delay module can be patterned at the bottom of the stack, and microfluidic modules which are utilized after the delay module (e.g., detection module and sorting module) can be patterned at the top of the stack.

Upon start-up, the hourglass will be stop-cocked to allow droplets to fill until the desired delay time is reached and then droplet will be removed from the device at the same rate that they enter, thereby ensuring essentially the same residency time for all droplets. Spontaneous droplet coalescence in the hourglass can be prevented by using one or more surfactants to stabilize the droplets.

The shape and timing of electric field gradients through the use of computer modeling can be optimized by tailoring the geometry of the electrodes and the fluid channels and the synchronization of the applied voltages to the droplets.

The FEMLAB (COMSOL, Inc.) partial differential equation solver software can be used to model the combination of fluid dynamics and electrostatics. The model can include “still-frame captures” of the trajectory of droplets through bifurcations, and can optimize the electrode geometry, the fluid channel geometry, and the distribution of applied voltages as a function of the incremental droplet trajectory. Further, a high-speed digital camera and driving electronics can be used to acquire “still-frame captures” of the actual droplet trajectories and comparing those captures to those produced by the model. The model and the electrode and fluid channel geometries can be iteratively optimized using inexpensive rapid prototyping capability (24 hours from design to test-results). Finally, the electric field gradients can be satisfactorily optimized when bidirectional sorting at rates of 1000 droplets/second or greater, without breaking the droplets and with an acceptably low error rate for the given application, is achieved. If the electromechanical relay network is not fast enough to operate with the optimized timing parameters, a solid-state relay network (e.g., using Behlke electronic relays) can be used to increase the speed of the driving electronics.

Droplets containing beads can be sorted using dielectrophoretic and electrostrictive forces based on a fluorescence probe at rates of 1000 droplets/s or greater. A fluorescence detection system and Electrical Control System can be used to trigger the optimal “pulse” (i.e., distribution of applied voltages as a function of time) to sort neutral droplets based on the fluorescence probe. Dielectrophoretic/electrostrictive sorting of droplets containing fluorescent dye can be performed, wherein the sorting is triggered by the droplet number (e.g., every nth droplet is sorted in one direction, or every nth or mth droplet is sorted in one direction, etc.). Fluorescent dye can be used to perform dielectrophoretic sorting of droplets because it is convenient and inexpensive; the trigger signal for the dielectrophoretic/electrostrictive sorting can be exactly the same as was used for electrophoretic sorting. This process is the direct logical consequence of optimizing the electric field gradients.

Additionally, dielectrophoretic/electrostrictive sorting of droplets containing fluorescent beads can be performed. This step is intermediate between droplets containing fluorescent dye and droplets containing cells and beads laden with chemical libraries. Finally, dielectrophoretic/electrostrictive sorting of droplets containing fluorescent cells can be performed. This step is intermediate between droplets containing fluorescent dye and droplets containing cells and beads laden with chemical libraries.

In the event that the solutions containing the beads or cells have dielectric properties so different than the solution containing fluorescent dye that the dielectric field gradients are not optimal, the dielectric field gradients can be optimized separately for each solution. The fluorescent dye solution can be modified to better resemble the bead or cell

solutions in order to continue to take advantage of the convenience of the fluorescent dye for the development of the sorting parameters.

Droplets sorted based on a particular phenotype (for example, dead cells) will be decoded (by using a decoding scheme) to identify the compound added in that droplet.

In some embodiments, the assay can be based on a nucleic-acid based encoded bead system. Two types of beads can be used for example—one contains a cytotoxic compound and oligonucleotide tag, and a second bead contains only a different oligonucleotide tag. The two types of beads may (optionally) also be encoded by a different fluorescent tag (i.e., other than the ones being used for the cell-based assays, as an example, two different Q-dots) so that the beads can be examined under a fluorescent microscope after sorting to determine the sorting efficiency.

The sorted beads from dead-cell containing nanoreactors can then be taken, and using the polymerase chain reaction (PCR), the tags on the beads can be amplified using PCR primers. These tags can be 'hard-copied' by cloning them into a plasmid vector, transforming them into *E. coli*, and the tag sequence of 100 different *E. coli* transformants determined by DNA sequencing.

Additionally, more complex libraries using T-bag synthesis on beads, can be constructed, wherein oligonucleotide tags are specific for each round of synthesis for a monomer. The same monomer used in two different rounds can have two separate tags. As a non-limiting example, if 30 monomers in a bead-based T-bag synthesis were used for 5 rounds, 5×30, or 150 different tags will be required. The complexity of a library of 30 monomers after 5 rounds is 30, or nearly 25 million compounds. The beads in a specific T-bag after each round of monomer synthesis can have a specific oligonucleotide tag ligated, using T4 DNA ligase, onto the beads. These tags, from sorted beads, can be amplified, cloned and sequenced. By knowing what tags were used in which round of synthesis, an internal check of validation of the bead that was positive in that droplet is achieved. The sequencing reaction can be eliminated by using a hybridization chip containing the 150 tags.

Example 2

The present invention provides methods for performing polymerase chain reaction in nanoreactors of the present invention as described. PCR can be performed on a drop-by-drop basis in a microfluidic device according to the present invention. A monolithic chip can be provided wherein the heating and cooling lines are built into the chip and a sorting means is provided. Advantages of performing PCR in droplets on such a chip are that the chip is disposable and the reaction can be repeated without cleaning the device between reactions. Furthermore, the chip provides a convenient way of getting all the components to perform PCR in the droplets in the right concentration. Additionally, the PCR is more efficient because the heat transfer is more efficient due to the small volume. This provides for shorter incubation/residence times. Droplets containing the nucleic acids, all PCR primers, and, if present, beads are generated one at a time at rates between 100 and 20,000 droplets per second. The droplets can then be sent through a serpentine path between heating and cooling lines to amplify the genetic material inside the droplets. Upon exiting the device the droplets may be sent for further on-chip or off-chip processing, directed into another chip, or the emulsion may be broken to release the PCR product. If present, beads may be

harvested by passing' the emulsion through a filtration device, sedimentation, or centrifugation.

The width and depth of the channel can be adjusted to set the residence time at each temperature, which can be controlled to anywhere between less than a second and minutes. At a typical rate of 1000 drops per second, 1 million strands of DNA can be amplified in approximately 20 minutes on one device. A typical flow rate of 250 μL/hour would correspond to 1000 drops of 50 microns in diameter being generated every second. Flow rates and droplet sizes can be adjusted as needed by controlling the nozzle geometry.

In an example bead based application, the purpose is to amplify at most one DNA fragment in a droplet containing a single micro-bead (1 to 100 microns in diameter) and then separate and collect only the beads coated with DNA. This is achieved by starting with a dilute mixture of DNA fragments and beads in a solution containing the appropriate PCR primers. Droplets are then made in the limited dilution regime where most of the droplets are empty, but some droplets have a DNA strand in them and some droplets have beads in them. The target droplets have both a single DNA fragment and a single bead. After PCR amplification of the DNA on the surface of the beads a fluorescence activated sorting module (NanoFACS) can be added to the end of the device to separate the droplets into two populations, one containing amplified DNA and one without amplified DNA. The beads are then removed from the emulsion where the droplets all contain DNA to achieve a collection of beads where essentially all beads are coated with only one type of DNA fragment.

The quality of the collection of beads where each fragment is amplified in the presence of only one bead can be enhanced by ensuring that each droplet contains at most one bead. Droplets containing more than one bead can be removed using a fluorescence-based sorting step.

Along with PCR, nucleic acid based signal methods such as tyramide assays using an appropriate enzyme reaction, oligonucleotides decorated with two or more detecting groups, or other amplification means, for example, rolling circle amplification, ligase chain reaction, and NASBA can be used to increase the signal within a droplet.

Example 3

The device of the present invention can be used to screen chemical libraries composed of at least 10⁶ molecules against an established cell line. In this manner, positive and negative nanoreactors can be tracked and sorted using either a nucleic-acid based, or multicolored bead-based encoding scheme. For example, a control library with known hits can be screened against a human cancer cell line.

In one embodiment, a chemical library can be screened using a nanoreactor as described in detail herein. The power of the present invention comes from a combination of compartmentalization and electrical manipulation that enables multi-step chemical processing, including analysis and sorting, to be initiated in confinement with exquisite timing and metering precision. This multi-step processing of isolated components is essential for searching through molecular libraries for rare interactions with cells, nucleic acids, enzymes, coded microbeads, and other biomaterials. For example, a set of encoding nucleic acids, (i.e., DNA tags) can be combined into solutions of unique chemical compounds such that the DNA tags and chemicals are emulsified together. In one embodiment, the DNA tag acts as a surrogate identifier to track the associated chemical compound in droplets sorted by a nanoreactor described herein.

After sorting, the emulsion can be broken and the nucleic acids can be decoded (FIG. 4). As shown in FIG. 4 (Left panel), (A) An individual compound from a library of compounds will each be combined (B) with a unique, differentiable set of q-dots. The combined mixture will each (C) be separately emulsified off-line using a flow-focusing microfluidics emulsifier to synthesize individual droplets containing both a specific compound and a unique set of q-dots. As shown in FIG. 4 (Right panel), the set of individually-emulsified encoded compounds will be (D) pooled together and injected, along with either cells or enzymes, into the RDT instrument and (E) the two droplets combined to form individual NanoReactors. Depending on the reaction being monitored, a separate combining (not shown in the figure) of these nanoreactors with droplets containing assay components may be needed. In addition, a delay loop may be placed between these combinings and the detector (F) to allow sufficient time to occur in the droplet as to allow any potential chemical/cellular/enzymatic reaction to occur. The nanoreactors are next sent past a detector to both monitor the reaction and decode the q-dots contained within it. The nanoreactors can be further sorted (G) if necessary. In designing the device to be placed on the Instrument, individual modules are strung together in a sequence of droplet operations. Operations can be used to encapsulate cells or enzyme, inject the labeled preformed compound library emulsion, coalesce pairs of droplets, mix the contents of droplets, incubate reactions over time, detect fluorescence, decode the liquid label, sort (if needed) based on the detected signal, and transport droplets to collection and waste streams. The individual modules operate independently, much like resistors and capacitors in an electrical circuit, to collectively perform complex fluid processing operations. Several methods encompassing various chemical library screening embodiments of the invention as described. In one example, a kinase enzyme assay is used as an enzyme model, three different quantum dots (q-dots) for the liquid label, and a set of 96 different chemical compounds (in which 1-2 will be preferred kinase substrates) as the library. Fluorescence polarization is preferred since the argument can be made that it can be adapted to many different types of assays. In one example, water-soluble q-dots that emit at 620 nm, 650 nm and 680 nm are used. These emission bands are well outside of spectral region where the target enzyme assays emit (below 580 nm), so these q-dots are an excellent choice for In another example, near-IR q-dots are used to enhance their water solubility for the purpose of expanding the non-overlapping spectral region of the target assays. Moving the q-dot readout to this "unused" wavelength band can permit virtually any fluorescence assay of interest to be adapted to the nanoreactors of the present invention without modification, tremendously expanding the application space immediately available.

The nucleic acid can be a linear molecule wherein the ends can be used as priming sites for PCR, and the middle sequence is unique to each chemical compound; it is this middle sequence that is used as the encode. The nucleic acid and chemical compound are together combined into one droplet by pre-emulsifying the nucleic acid and chemical together and then adding them to a microfluidic device as described herein, as a pre-made, compound droplet. The compound droplet can be combined with a another droplet on the instrument. This other droplet can contain an item under investigation (including for example, but not limited to, a cell or enzyme), which, when combined with the compound droplet forms an 'assay' droplet. The assay droplets having a desired detected property (for example,

inhibition of enzyme activity through the use of a fluorescent substrate added to the compound microdrop) can then be sorted. The sorted assay droplets can be collected, the emulsion broken, and the nucleic acid sequence can be decoded. The decoding can be performed by emulsion PCR (as described in U.S. Application Publication No. 2005-0227264) and sequencing on a sequencing instrument. Alternatively, the decoding can be performed by cloning the PCR product into an appropriate host (for example, *E. coli*), and the resultant clones subjected to DNA sequencing.

The nucleic acid can be a linear molecule having a region of uniqueness, and the decoding can be performed by cloning and subsequently transforming the DNA obtained from sorted assay droplets into an appropriate host {e.g., *E. coli*). The resultant clones can then be subjected to decoding by hybridizing a PCR product containing the unique identifier to a complementary strand of nucleic acid fixed to a solid support (for example a chip, wafer, or bead).

The nucleic acid can be a plasmid having a region of uniqueness, and the decoding can be performed by transforming the DNA obtained from sorted assay droplets into an appropriate host {e.g., *E. coli*). The resultant clones can then be subjected to DNA sequencing to identify the encoded sequence. The nucleic acid can be a plasmid having a region of uniqueness, and the decoding can be performed by transforming the DNA obtained from sorted assay droplets into an appropriate host (e.g., *E. coli*). The resultant clones can then be subjected to decoding by hybridizing a labeled-PCR product containing the unique identifier to a complementary strand of nucleic acid fixed to a solid support (for example a chip, wafer, or bead).

The nucleic acid can be either a plasmid or linear fragment having a region of uniqueness, and the decoding can be performed by transforming the DNA obtained from sorted assay droplets into an appropriate host (e.g., *E. coli*). The resultant clones can then be subjected to decoding by hybridizing a labeled-PCR product containing the unique identifier to a complementary strand of nucleic acid fixed to a solid support (for example a chip, wafer, or bead). Preferably, the bead can be encoded with dyes or Qdots, and the decoding can be performed on a microfluidic device according to the present invention, or on a Qdot or Luminex installment.

A set of unique nucleic acids can be added to a set of unique chemical entities, wherein each combined set is separately emulsified. The separately emulsified combined set can be further combined to generate an emulsified mixed solution of droplets, wherein each droplet can contain both a nucleic acid and a unique chemical entity. This combined mixed solution can be injected into a microfluidic device according to the present invention for use in various assays contemplated by one of ordinary skill in the art.

The nucleic acid containing unique identifiers can be generated by PCR of an antibiotic resistance or other selectable gene with a set of the forward and reverse PCR primers each containing a 5' nucleotide sequence common to each other, forward and downstream primers, respectively, a unique sequence 3' to the common sequence, and a region of the antibiotic or other selectable gene. Said primers can be used in a PCR reaction to generate an antibiotic resistance or other selectable gene bracketed by unique identifiers which in turn can be bracketed by either a forward or reverse common sequence. The PCR product can then be cloned into a vector having a second antibiotic resistance or other selectable gene, and the vector can be cloned into an appropriate host (e.g., *E. coli*), thereby selecting for antibiotic resistance and another selectable gene simultaneously.

The label can also be a solution containing a dye such as an organic dye (for example cy3, cy5, fluorescein) or inorganic label such as a quantum dot. The dot can be further coated or encapsulated by hydrophobic residues. More than one dye can be added to a solution prior to emulsification and the ratio of one or more dyes can be used to decode the droplet.

Additionally, many bead-encoded assays have already been developed for microspheres that should be directly ported to the devices and systems disclosed herein. Such assays include, for example: allergy testing, disease markers (including, autoimmune, cancer and cardiac), cytokine, genotyping, gene expression, infectious disease, kinase/phosphorylated proteins, metabolic markers, tissue typing, transcription factors/nuclear receptors and others.

The present invention also provides methods of using a drop-washer for combinatorial chemistry/biology. A device of the present invention capable of exchanging constituents within a droplet through the use of fluid flow in such a way that the microdrop, while in a first immiscible fluid, is exposed to a second immiscible fluid such that constituents within the droplet that are immiscible in the first immiscible fluid are soluble in the second immiscible fluid.

For example, an aqueous droplet containing a chemical reaction produces by-products that are soluble in a lipid solvent. The chemical reaction is performed in a water-environment in a silicon-based solvent. After the chemical reaction occurs, the droplet is exposed to an organic-oil based solvent where the chemical byproducts are allowed to diffuse out of the droplet. The resulting droplet is then assayed for cell-killing activity by combining the droplet with live cells.

Similar to the preceding example, but the change in the, non-aqueous fluid flow is used to add a particular constituent from the second immiscible fluid to diffuse into the aqueous drop before the droplet is returned to the 100% first immiscible fluid flow.

Example 4

The present invention also provides methods of performing biological assays in nanoreactors using fluorescence polarization (FP). Fluorescence polarization technology has been used in basic research and commercial diagnostic assays for many decades, but has begun to be widely used in drug discovery only in the past six years. Originally, FP assays for drug discovery were developed for single-tube analytical instruments, but the technology was rapidly converted to high-throughput screening assays when commercial plate readers with equivalent sensitivity became available. These assays include such well-known pharmaceutical targets such as kinases, phosphatases, proteases, G-protein coupled receptors, and nuclear receptors.

Nuclear Receptors;

FP has been used to develop high throughput screening (HTS) assays for nuclear receptor-ligand displacement (Parker G J, et al, Development of high throughput screening assays using fluorescence polarization: nuclear receptor-ligand-binding and kinase/phosphatase assays). The FP-based estrogen receptor (ER) assay is based on the competition of fluorescein-labeled estradiol and estrogen-like compounds for binding to ER. In a screen of 50 lead compounds from a transcriptional activation screen, 21 compounds had IC50 values below 10 microM, with one exhibiting roughly a 100-fold higher affinity for ERbeta over

ERalpha. An FP-based competitive binding assay can be used to screen diverse compounds with a broad range of binding affinities for ERs.

Phosphatases and Kinases;

A nonradioactive, simple, sensitive fluorescence polarization assay has been developed to assay protein tyrosine kinase activity (Seethala R.; Menzel R. A Homogeneous, Fluorescence Polarization Assay for Src-Family Tyrosine Kinases. *Analytical Biochemistry*, November 1997, vol. 253, no. 2, pp. 210-218(9)). This assay involves incubation of a fluorescenyated peptide substrate with the kinase, ATP, and anti-phosphotyrosine antibody. The phosphorylated peptide product is immunocomplexed with the anti-phosphotyrosine antibody resulting in an increase in the polarization signal as measured in a fluorescence polarization analyzer. These results show that the fluorescence polarization assay can detect inhibitors and is comparable to the 32 PO 4 transfer assay. The fluorescence polarization method is advantageous compared to the 32 PO 4 transfer assay or ELISA or DELFIA because it is a one-step assay that does not involve several washings, liquid transfer, and sample preparation steps. It has the added advantage of using nonisotopic substrates. The fluorescence polarization assay thus is environmentally safe and minimizes handling problems.

G-Protein Coupled Receptors;

High-throughput fluorescence polarization (FP) assays offer a nonradioactive, homogeneous, and low-cost alternative to radioligand binding assays for cell surface receptors (G protein-coupled receptors and ligand-gated ion channels) (Allen M, Reeves J, Mellor G. High throughput fluorescence polarization: a homogeneous alternative to radioligand binding for cell surface receptors. *J Biomol Screen*. 2000 April; 5(2):63-9). FP assays were shown to work across a range of both peptide (vasopressin Via and delta-opioid) and non-peptide (beta 1-adrenoceptor, 5-hydroxytryptamine3) receptors. Assays could be run in 384-well plates with little loss of signal window or sensitivity compared to 96-well plate assays. New advances in FP measurement have therefore enabled FP to offer a high throughput alternative to radioligand binding for cell surface receptors.

GTPases;

A 30,000-member compound library was screened using filter binding [FB (33 P)] and FP detection systems, and compounds that were active in either assay were retested in 5-point curve confirmation assays (CL. Hubert et al. Data Concordance from a Comparison between Filter Binding and Fluorescence Polarization Assay Formats for Identification of ROCK-II Inhibitors). Analysis of these data showed an approximate 95% agreement of compounds identified as active in both assay formats. Also, compound potency determinations from FB and FP had a high degree of correlation and were considered equivalent. These data suggest that the assay methodology has little impact on the quality and productivity of the screen, provided that the assays are developed to standardize kinetic conditions.

Diagnostics Using Antibodies;

The control of equine infectious anemia virus (EIAV) infections of horses has been over the past 20 years based primarily on the identification and elimination of seropositive horses, predominantly by a standardized agar gel immunodiffusion (AGID) assay in centralized reference laboratories. Peptides derived from antigenic regions of EIAV core and envelope proteins were initially screened for their utility as probes in an FP assay to select the best peptide antigen candidates (S. B. Tencza, et al. Development of a Fluorescence Polarization-Based Diagnostic Assay for Equine

Infectious Anemia Virus. *Journal of Clinical Microbiology*, May 2000, p. 1854-1859, Vol. 38, No. 5). The FP assay was optimized to detect the presence of EIAV-specific antibodies by a change in the FP of a fluorescein-labeled immunoreactive peptide diagnostic antigen. The most sensitive and specific peptide probe was a peptide corresponding to the immunodominant region of the EIAV transmembrane protein, gp45. This probe was tested for its reactivity in the optimized FP assay with 151 AGID-positive horse sera and 106 AGID-negative serum samples. The results of these studies demonstrated that the FP assay reactivity correlated with reported AGID results in 106 of 106 negative serum samples (100% specificity) and in 135 of 151 positive serum samples (89.4% sensitivity). The FP assay was also found to have a very low background reactivity and to readily detect antibodies produced early in infection (<3 weeks postinfection).

FP is a homogeneous technology with very rapid reactions; seconds to minutes suffice to reach equilibrium. As the reagents are stable, large highly reproducible batches may be prepared. Because of these properties, FP has proven to be highly automatable, often performed with a single incubation with a single, premixed, tracer-receptor reagent. The fact that there are no washing steps increases the precision and speed over heterogeneous technologies and dramatically reduces waste.

Other homogeneous technologies based on fluorescence intensity have been developed. These include energy transfer, quenching, and enhancement assays. FP offers several advantages over these. The assays are usually easier to construct, since the tracers do not have to respond to binding by intensity changes. In addition, only one tracer is required and crude receptor preparations may be utilized. Furthermore, since FP is independent of intensity, it is relatively immune to colored solutions and cloudy suspensions. FP offers several advantages in the area of instrumentation. Because FP is a fundamental property of the molecule, and the reagents are stable, little or no standardization is required. FP is relatively insensitive to drift in detector gain settings and laser power.

The concept of molecular movement and rotation is the basis of fluorescence polarization. By using a fluorescent dye to label a small molecule, its binding to another molecule of equal or greater size can be monitored through its speed of rotation. As shown in FIG. 5, dye molecules with their absorption transition vectors (arrows) aligned parallel to the electric vector of linearly polarized light (along the vertical page axis) are selectively excited. For dyes attached to small, rapidly rotating molecules, the initially photoselected orientational distribution becomes randomized prior to emission, resulting in low fluorescence polarization. Conversely, binding of the low molecular weight tracer to a large, slowly rotating molecule results in high fluorescence polarization. Fluorescence polarization therefore provides a direct readout of the extent of tracer binding to proteins, nucleic acids and other biopolymers.

Fluorescence polarization, first described in 1926 by Perrin, has a long history. FP theory and the first instrument for measuring was developed by Weber. This work was expanded to biological systems, such as antigen-antibody reactions and hormone-receptor interactions by Dandliker. The first commercial systems, aimed at monitoring drugs in body fluids come from Jolley and co-workers.

Fluorescence polarization is defined by the following equation: $P=(V-H)/(V+H)$ where P is the polarization unit, V is the intensity of the vertical component of the emitted light, and H is the intensity of horizontal component of the

emitted light of a fluorophore excited by vertical plane polarized light. The "polarization unit" P is a dimensionless entity and is not dependent on the intensity of the emitted light or on the concentration of the fluorophore. This is the fundamental power of FP. The term "mP" is now in general use, where 1 mP equals one thousandth of a P.

The excitation dipole is the direction in which the molecule prefers to absorb light. The emission dipole is the direction in which a molecule prefers to emit light. This assumed (for the sake of simplicity) that these directions are parallel. In one experiment, if the fluorescent molecules are fixed so that all excitation dipoles are aligned in the vertical plane and assume there is only fluoresces with a polarization along the emission dipole then a maximum polarization unit of 1000 mP is observed. If, however, the excitation dipoles were randomly oriented this maximum polarization unit is reduced to 500 mP. In another experiment, if the requirement that the dipoles are fixed was removed and they are allowed to reorient between the time when they are excited and the time when they fluoresce the polarization unit falls below 500 mP.

In another experiment, a collection of randomly oriented transition moments are free to rotate. In this case, the polarization unit is between 0 and 500 mP and is dependent on how far the molecule has rotated during the fluorescence lifetime of the excited state. The smaller the molecule, the faster it rotates, and so the lower the FP will be. The rate of rotation of a molecule is described by the Stokes equation: $\rho=(3\eta V)/(RT)$ where ρ is the rotational relaxation time (the time required to rotate through an angle whose cosine is $1/e$, or approximately 68.5°), η is the viscosity of the medium, V is the molecular volume of the molecule, R is the gas constant, and T is the temperature in degrees Kelvin. From the previous equations we can see that the higher the molecular weight of a molecule, the higher the rotational relaxation time will be; $V=vM$ where M (Perrin equation) is the molecular weight of the molecule in Daltons and v is its partial specific volume ($\text{cm}^3 \text{g}^{-1}$). The Perrin equation was first described in 1926, and describes the relationship between the observed FP, the limiting polarization, the fluorescence lifetime of the fluorophore (τ), and its rotational relaxation time. $((VP)^{-1/3})=((1/P_o)^{-1/3})\times((1+(3\tau/P))$.

The shorter the fluorescence lifetime, the higher the FP will be. Conversely, the shorter the rotational relaxation time, the smaller the FP will be. Combining the Stokes equation and the Perrin equation, and substituting M for V and rearranging, we get the relationship between the molecular weight of a molecule and its FP (1/P is proportional to 1/M); $(1/P)=(1/P_o)+((1/P_o)^{-1/3})\times(RT/vM)\times(\tau/\eta)$. From this equation we can see that P equals P_o in the limiting cases of high molecular weight, high viscosity, and short lifetime. In fact, P_o can be determined by measuring FP at various viscosities, plotting P against $1/\eta$, and determining the intercept on the ordinate.

Organic fluorophores have characteristics, such as narrow excitation bands and broad red-tailing emission band. FIG. 6 (Left, Center Panel) shows the absorption and emission spectra of q-dot 535 nanocrystals and fluorescein, respectively. FIG. 6 (Right panel) shows the emission spectra of several sizes of CdSe—ZnS quantum dots, with excitation of ZhSe at 290 nm, all others at 365 nm in all cases. These bands often limit their effectiveness. This makes concurrent resolution of multiple light-emitting probes problematic due to spectral overlap. Also, many organic dyes exhibit low resistance to photodegradation.

Luminescent colloidal semiconductor nanocrystals called quantum dots or q-dots (QD) are inorganic fluorophores that

have the potential to circumvent some of the functional limitations encountered by organic dyes. In particular, CdSe—ZnS core-shell QDs exhibit size-dependent tunable photoluminescence (PL) with narrow emission bandwidths (FWHM ~30 to 45 nm) that span the visible spectrum and broad absorption bands. These allow simultaneous excitation of several particle sizes (colors) at a common wavelength. This, in turn, allows simultaneous resolution of several colors using standard instrumentation (FIG. 6, right panel). CdSe—ZnS QDs also have high quantum yields, are resistant to photodegradation, and can be detected optically at concentrations comparable to organic dyes.

Quantum dots are nano-scale semiconductors typically consisting of materials such as crystalline cadmium selenide. The term ‘q-dot’ emphasizes the quantum confinement effect of these materials, and typically refers to fluorescent nanocrystals in the quantum confined size range. Quantum confinement refers to the light emission from bulk (macroscopic) semiconductors such as LEDs which results from exciting the semiconductor either electrically or by shining light on it, creating electron-hole pairs which, when they recombine, emit light. The energy, and therefore the wavelength, of the emitted light is governed by the composition of the semiconductor material. If, however, the physical size of the semiconductor is considerably reduced to be much smaller than the natural radius of the electron-hole pair (Bohr radius), additional energy is required to “confine” this excitation within the nanoscopic semiconductor structure leading to a shift in the emission to shorter wavelengths.

Fluorescence polarization assays can be used in a microfluidics device to monitor the activity of kinase enzymes, phosphatases, proteases, ligand-ligand binding, and others. Extension of the existing fluorescence detection system to perform fluorescence polarization measurements requires the incorporation of a linearly polarized laser and polarizing optics into the design. As shown in FIG. 7, linearly polarized laser and polarizing optics is incorporated into the design. A linearly polarized frequency doubled diode laser operating at 488 nm passes through a 1/2 waveplate and linear polarizer (Meadowlark Optics, >2000:1 contrast ratio). This makes it possible to orient and lock the exciting laser polarization as required for FP. The laser is reflected and focused into the sample using a dichroic beamsplitter and anti-reflection coated lenses. Fluorescence from the sample is transmitted back through the lenses and dichroic beamsplitter and isolated using the emission filter. This fluorescence signal is then split into orthogonal polarizations using a polarizing beamsplitter (Meadowlark Optics polarizing cube beamsplitter, contrast ratio >500:1 transmitted, >20:1 reflected). Contrast is further enhanced with linear polarizers (Meadowlark Optics, >2000:1 contrast ratio). Finally, each polarization signal is measured using a pair of photomultiplier tubes (Hamamatsu H5789), digitized and analyzed by computer. A linearly polarized (>200:1) frequency doubled diode laser operating at 488 nm from Picarro is used for this purpose. As seen in the figure, the laser passes through a Vt waveplate and linear polarizer (Meadowlark Optics, >2000:1 contrast ratio). This makes it possible to orient and lock the exciting laser polarization as required for FP. As with the standard station, the laser is reflected and focused into the sample using a dichroic beamsplitter and anti-reflection coated lenses. Fluorescence from the sample is transmitted back through the lenses and dichroic beamsplitter and isolated using the emission filter. This fluorescence signal is then split into orthogonal polarizations using a polarizing beamsplitter (Meadowlark Optics polarizing cube beamsplitter, contrast ratio >500:1 transmitted, >20:1

reflected) and contrast is further enhanced with linear polarizers (Meadowlark Optics, >2000:1 contrast ratio). Finally, each polarization signal is measured using a pair of photomultiplier tubes (Hamamatsu H5789), digitized and analyzed on the computer. It is expected that these optics will permit better than mP sensitivity.

These fluorescence polarization systems were tested using a model enzyme system; Src-family tyrosine kinase. A nonradioactive, simple, sensitive fluorescence polarization assay has been developed to assay protein tyrosine kinase activity (Seethala R.; Menzel R. A Homogeneous, Fluorescence Polarization Assay for Src-Family Tyrosine Kinases. *Analytical Biochemistry*, November 1997, vol. 253, no. 2, pp. 210-218(9)). This assay involves incubation of a fluorescenyated peptide substrate with the kinase, ATP, and anti-phosphotyrosine antibody. As shown in FIG. 8, the phosphorylated peptide product is immunocomplexed with the anti-phosphotyrosine antibody resulting in an increase in the polarization signal as measured in a fluorescence polarization analyzer. FIG. 8, left panel, shows the IMAP principle of operation. When a fluorescent substrate is phosphorylated by a kinase, it can bind to the IMAP binding reagent, whose molecular size is large relative to the substrate. This gives a large increase in the polarization of the fluorescence. FIG. 8, middle panel, shows the IMAP assay of MAPKAP-K2, a serine/threonine kinase. MAPKAP-K2, from Upstate, was assayed in a volume of 20 μ L using the amounts of enzyme indicated. Concentrations of ATP and substrate were 5.0 and 0.5 μ M, respectively. Incubation was 60 minutes at room temperature, followed by the addition of 60 μ L IMAP binding reagent. FP was read on an Analyst system 30 minutes later. FIG. 8, right panel, shows the IMAP quantification of kinase inhibition. MAPKAP-K2 (0.25 units/mL) was incubated using the amounts of enzyme shown for 15 minutes. The activity of the enzyme was then assessed as described in above. These results show that the fluorescence polarization assay can detect inhibitors and is comparable to the $^{32}\text{PO}_4$ transfer assay. The fluorescence polarization method is advantageous compared to the $^{32}\text{PO}_4$ transfer assay or ELISA or DELFIA because it is a one-step assay that does not involve several washings, liquid transfer, and sample preparation steps. It has the added advantage of using nonisotopic substrates. The fluorescence polarization assay thus is environmentally safe and minimizes handling problems.

The dyes that are chosen are used extensively in flow cytometry and in our instrument will be determining the status of (potentially) many dyes within one drop. The use of inexpensive optics on our instrument will be more than compensated for by the theoretical increase of dye molecules in the nanoreactor.

FP assays have been shown to tolerate up to 5% DMSO with no loss in sensitivity or signal window. From a random set of 1,280 compounds, Allen et al found that 1.9% significantly interfere with FP measurement (*J Biomol Screen.* 2000 April; 5(2):63-9. High throughput fluorescence polarization: a homogeneous alternative to radioligand binding for cell surface receptors. Allen M, Reeves J, Mellor G. Receptor & Enzyme Screening Technologies, Glaxo Wellcome Medicines Research Centre, Stevenage, Herts, UK.). If fluorescent or quenching compounds were eliminated (3% of all compounds), less than 0.4% of compounds were found to interfere with FP measurement. Compounds are assayed a priori and those that have these undesirable characteristics are eliminated.

In some enzymatic assays, a delay module (i.e., delay line) will be utilized. This is less true for enzyme reaction

mechanisms in a small volume. And even many cell-based assays can be measured within 5 minutes. Longer assay times can be accomplished by collecting the droplets, incubating them for an appropriate amount of time, and then re-injecting them into the device.

Three different q-dots in several concentrations each can be placed in a microdroplet, and can then be used with the device of the present invention to decode what is in the drop. In one experiment, the initial labeling scheme used three colors of q-dots having emission wavelengths of 620 nm (CdSe/ZnS), 650 nm (InGaP/ZnS), and 680 nm (InGaP/ZnS) (excitation at 488 nm is appropriate for all). In one specific example, one q-dot was maintained at a constant concentration and varying the second and third q-dots at least 10 different concentrations giving 100 different encodes (1×10×10). Decoding will be computed by referencing the intensity of the second and third q-dots relative to the first q-dot. Other labeling schemes can be used during the course of these experiments.

The Q-dot readout extension to the fluorescence station is described herein and is easily incorporated into the design due to the modular layout developed. As seen, a series of dichroic beamsplitters, emission filters, and detectors are stacked onto the system, allowing measurement of the required five emission channels (two fluorescence polarization signals and three q-dot bands). Dichroic beamsplitters and emission filters capable of separating the q-dot wavelength bands from each other are readily available, so it is a straightforward process to configure the station appropriately.

The residence time can be increased by slowing down the flow of drops by widening the channel. Alternatively the intensity of the laser beam can be increased to compensate or increase the concentration of the q-dots within the droplet.

As described herein, the dyes chosen for FP are commonly used in most cell- and enzyme-based assays and are designed not to overlap significantly with the q-dots. The dyes are evaluated both independently and together with the q-dots (at first off-instrument) to assess the cross-talk. Preferably, the liquid q-dot labels are read outside a spectral wavelength band currently used in FACS analysis and sorting (i.e., the dyes fluorescein, Cy3, Cy5, etc). This permits the use of currently-available assays (dependent on these dyes). Using specific q-dots, crosstalk is minimized. Several commercial entities sell q-dots that can be read by the optics being designed. The three colors of q-dots used currently are the non-functionalized T2 EviTags having emission wavelengths of 620 nm (CdSe/ZnS), 650 nm (InGaP/ZnS), and 680 nm (InGaP/ZnS) (excitation at 488 nm is appropriate for all).

It is possible to generate 96 types of droplets, each droplet containing both a unique set of q-dot labels and a chemical compound, and as the droplet flows through the device of the present invention kinase enzyme activity can be analyzed using FP and the q-dot label can be decoded. This method allows for scaling to more complex and interesting libraries.

FP assays have been shown to tolerate up to 5% DMSO with no loss in sensitivity or signal window. From a random set of 1,280 compounds, Allen et al. found that 1.9% significantly interfere with FP measurement (J Biomol Screen. 2000 April; 5 (2): 63-9. High-throughput fluorescence polarization: a homogeneous alternative to radioligand binding for cell surface receptors. Allen M, et al. Receptor & Enzyme Screening Technologies, Glaxo Wellcome Medicines Research Centre, Stevenage, Herts, UK.). If fluorescent or quenching compounds are eliminated (3% of all compounds) then less than 0.4% of compounds are

found to interfere with FP measurements. Compounds are assayed a priori and those that quench FP are eliminated.

The three colors of q-dots we will use are the non-functionalized T2 EviTags having emission wavelengths of 620 nm, 650 nm, and 680 nm; excitation at 488 nm is appropriate for all. The >620 nm liquid labeling emission band was chosen not to interfere with the FP assay band found between 488 and 620 nm. These q-dots are commercially-available, stable in some buffers and remain suspended in aqueous solution.

A mixture of two types of droplets, buffer-only and fluorescein-containing, are stable for at least 1 month without any detectable diffusion of the organic dye into the buffer-only droplets. Other surfactants may be substituted for different kinds of compounds. For other compound testing, i) similar mixtures of compound-containing and buffer-only droplets can be created, ii) they can be sorted based on their q-dot labels, and iii) Mass Spectrometry can be used on the buffer-only droplets to quantitatively detect the presence of other chemicals compounds.

In some embodiments, a delay module (i.e., delay line) can be utilized. This will be true for enzyme reaction mechanisms in a small volume. But even many cell-based assays can be measured within 5 minutes. Droplets can also be taken off-line and stored for at least a month before re-injection into the device of the present invention with no apparent change in the droplets. Longer delay times can be achieved by taking mixed droplets offline, and then re-injected them.

Example 5

The present invention provides methods for performing condensation chemistry in nanoreactors of the present invention as described to synthesize libraries of drug-like molecules in a highly convergent manner.

All life processes can be reduced to chemical reactions that take place in aqueous media. Hence water is considered to be the universal ultimate solvent and inevitably biological experiments are performed in aqueous media. Furthermore, organic solvents of all types are detrimental to biochemical reactions limiting their use to small percentages of water miscible solvents such as dimethyl sulfoxide and ethylene glycol. On chip synthesis in our system therefore requires that all chemical reactions are performed in biologically compatible aqueous media. In contrast, conventional synthetic organic chemistry relies on highly activated substrates and highly reactive reagents to conduct bond forming processes. Typically these substrates and/or reagents are unstable in the presence of and react with water rendering them useless. An ever increasing effort to reduce cost, enhance safety and to address environmental concerns w.f.t. solvent choice has driven the development of synthetic methods that utilize water as the primary and in many cases the only solvent (Li). In the case in which water is not the only solvent, water miscible organic solvents are used to aid the dissolution of substrates.

While material can be removed from NanoReactors by breaking them in a controlled way, it is preferable to avoid having to do so. To eliminate the requirements of removing material from droplets, we have identified 5 reaction types, which can be performed in aqueous media, that can be used to "stitch" drug-like molecules together from a highly diverse library of sub-structural components. These reactions generate commonly occurring functional groups in drug-like molecules and include: i) N-Acylation ii) N-Sulfonylation iii) Cycloadditions iv) Reductive alkylation of

amines and v) SNAr reactions (Morgan). Random combination of sub-structures will yield a library of all possible combinations. The reactions are sufficiently orthogonal to perform multi-step reactions. Furthermore, simple protection and deprotection schemes can be used to increase the number of condensations. A sufficient number excess of component nanoreactors will yield a library of all possible combinations with multiple copies of each combination for testing in a biomolecular assay. This redundancy is required to reduce the impact of false positive sorting events.

This technology is based on the assembly of drug-like chemical entities by two or more step convergent syntheses from diverse sub-structural components. A two step process would assemble the final chemical species from four sub-structures. An example of such a synthesis is the construction of the kinase inhibitor Gleevec from relatively simple building blocks. Gleevec is the first of a class of kinase inhibitors which targets the chimeric tyrosine kinase bcr-abl. Bcr-abl is constitutively active causing a rare life-threatening form of cancer called chronic myeloid leukemia (CML). Gleevec was given FDA approval in a record breaking three months in May of 2001. Analogues to a sphere, the three dimensional structure can be broken down into hemispheres and quadrant by the appropriate disconnections. FIG. 9 shows that Quadrants A and B are combined utilizing a reductive alkylation. Quadrant C and D are combined utilizing a 1,3 dipolar cycloaddition. The Hemisphere AB and CD are combined utilizing an N-acylation

Chemical Diversity is achieved by varying the sub-structural units (Quadrants) and randomly combining to achieve all possible combinations. Table 1 shows the theoretical diversity for number of each quadrant (e.g. 4 different Quadrants A, with 4 different Quadrants B, with 4 different Quadrants C and 4 different Quadrants D yield 256 unique products after two steps as described above.

TABLE 1

Diversity of quadrants (equal number of diverse members for each quadrant)	Number of Unique solutions
1	1
2	16
3	81
4	256
5	625
6	1,295
7	2,401
8	4,096
9	6,561
10	10,000

Sufficiently diverse condensation chemistry in aqueous media exists to synthesize diverse-libraries of drug-like molecules in a highly convergent manner.

The majority of synthetic reactions routinely used in the synthesis of complex drug-like molecules rely on reagents and substrates which are sensitive to hydrolysis in the presence of water and hence require stringent exclusion of water from the reaction vessel. Furthermore, condensation reaction often require the equivalent of a dehydrator to proceed, with one or both of the condensation substrates being sensitive to degradation by water. The pursuit of "greener" chemistry, using benign and environmentally friendly solvents such as water, has resulted in the development of several condensation reactions which take place in the presence of water. Aqueous organic chemistry has been extensively reviewed in the primary literature and books.

The encapsulation technology of the present invention which relies on the addition of reagents and/or substrates to nanoreactors without the option for reaction work-up (i.e. purification of product). This precludes the use of reactions which have side products which could potentially interfere with subsequent steps or the biological assay intended to be performed on the final product. Furthermore, in multistep reactions, the two steps will have to be orthogonal with respect to their coupling chemistry, i.e. the functional groups for consecutive reactions may not interfere with each other. Five reaction types have been identified which can be performed in aqueous media and which do not require purification of the product prior to the next synthetic step or testing in biological assays. These reactions include: i) N-Acylation ii) N-Sulfonylation iii) Cycloadditions iv) reductive alkylation of amines and v) SNAr reactions.

The present invention provides methods of performing these condensation reactions in a highly convergent, "one pot" synthesis to stitch together complex drug-like molecules from at least 2-16 substructures.

The solubility of organic compounds in aqueous media is strongly dependent on their structure. To enhance solubility of the library compounds in aqueous media, it is common in the biomolecular screening community to dissolve library compounds in DMSO and subsequently dilute the DMSO solution with water. DMSO is compatible with the nanoreactors described herein.

A fluorescent product resulting from the condensation of two suitable fragments can be distinguished from droplets that have components which did not react to form the fluorescent product thus enabling the optical readout to distinguish between the two cases and sort the droplets accordingly. The components able to form the fluorescent product would contain a different tag from the components which are not able to form a fluorescent product. Hence this system can be used to test the tagging strategy chosen to identify the composition of the final product.

Traditional combinatorial chemistry relies on complex deconvolution methods to determine the structural identity of the final product once it has been determined to be active in any particular biomolecular assay. Massively parallel synthetic approaches use encoding technologies to infer the structure of any particular product from the tag associated with it which typically identifies the reaction history of that particular compound. In one example, the reagent droplets are encoded with nucleic acids tag which will provide a unique PCR signature for the final product from which the reactant composition and hence structure can be inferred.

The synthesis of a fluorescent molecule which will be the product of one particular component with a common reaction partner will be used to test the tagging technology. FIG. 10 shows three tags denoted A, B and C label one of each of the following unique components: A is a fragment which if combined with C will yield a fluorescent molecule. B is a fragment which if combined with C will yield a non-fluorescent molecule. The fluorescence detector will be able to distinguish between drops that contain A, B, C or the mixture BC and between the drops which contain the mixture AC (if the reaction has taken place and the fluorescent product is formed). The fluorescence based sorting will yield a population of AC tags which are completely devoid of B. The second (waste) population of drops may contain B, C and A tag if not every drop containing the tag A has been fused to a drop containing C.

Multistep convergent syntheses of drug-like compounds can be performed in nanoreactors by the selective fusion of

droplets. These compounds can then be tested in a biomolecular screen immediately after being synthesized on chip.

The synthesis of the bcr-abl kinase inhibitor Gleevec has been described herein. The synthesis of this inhibitor from four sub-structural units followed by an assay determining its ability to inhibit the bcr-abl kinase in a fluorescence polarization based assay would serve as proof of principle for this technology.

Two different sub-structures will be used for each quadrant such that at least 16 possible products can be formed of which one is Gleevec. Although some of the other products will have sub-structural elements of Gleevec, the "alternative" quadrants will be considerably different to ensure that a completely non-active product will be amongst the possible combinations. Each unique quadrant will be tagged with a suitable nuclei acid oligomer.

The products will be tested in a fluorescence polarization based kinase assay with the expectation that Gleevec will strongly inhibit the activity of bcr-abl. Based on the assay readout, the drops containing Gleevec will be sorted and collected separately. Analysis of the nucleic acid tags of those drops can reveal the composition of the hit compound.

The present invention also provides methods of using nucleic acids for chemical encoding and decoding tagging of chemical reactions. Current technology exists for the tagging of beads with chemical tags which "record" the synthetic history of any particular bead thereby allowing the deconvolution of the active small molecule's structure. The encapsulation of the reagents used to assemble the library members enables the use of homogeneous nucleic acid based tags to determine the structure of any particular quaternary reaction combination. Positive hits from the biomolecular screen would be cloned into *E. coli* and decoded using polymerase chain reaction (PCR) to determine the composition of quadrants used to assemble the bio-active molecule. FIG. 11 (left panel) shows four groups of DNA tags. One of sixteen double-stranded oligodeoxynucleotide 'surrogate' tags will be added to each of four 'groups' of the sixteen different chemicals being used for chemical synthesis (see text for details). Each group of tags will have unique overlapping 5' and 3' ends that are the same for each member of the group, but complementary between adjacent groups. The tags within the groups are designed with asymmetric 5' overhangs such that they can ligate once with a member of an adjacent group. The first and fourth groups will additionally contain 5' and 3' sequences (respectively) that can be used as priming sites to PCR up final products containing all four groups. The top-strand in groups 2, 3 and 4 will contain a 5' phosphate needed for DNA ligation. FIG. 11 (right panel) shows the tags in each reaction are sorted based on the enzyme assay. In the example shown, chemical synthesis is allowed to occur (see text for details) and droplets (in this example) containing tags 2, 7, 11 and 14 have within them a synthesized compound that reacts positively in an enzyme/cell-based assay. The positive droplets are then subjected to a polymerase chain reaction (PCR) using primers complementary to the ends of groups 1 and 4. The resulting PCR product will next be cloned into an appropriate DNA vector. Finally, colonies of transformed *E. coli* containing the catenated tags will be DNA-sequenced to decode the synthesis history of the compound associated with positively-sorted droplets.

Alternatively soluble quantum dot dyes can be used to encode the input emulsions which can identify the chemical composition of a positive hit by measuring relative fluorescence signals of multicolored quantum dots eliminating the need for sorting. An assay point with appropriate signal from

a fluorescent marker (in the case of the kinase assay proposed here we would measure changes in fluorescence polarization) the synthetic history of the molecule responsible for this signal would be read out by determining relative levels of dyes. This tagging technology is limited by the number of unique combinations that can be discerned with appropriate confidence and hence would be applied to smaller, more focused libraries typically used to explore a sub-set of chemical space surrounding an early lead.

Example 6

The present invention provides methods of isolating self-antigens. A first sample droplet set consisting of a tumor obtained from a multicellular organism treated in such a way as to create single cells that are then each separately or multiply contained within said first droplet set are combined with a second set of droplets consisting of one or more t-cells isolated from the organism, and the resulting combined droplets are analyzed for t-cell killing of the tumor cells contained within the combined droplets using a detecting means. The detecting means can include analysis for cytoplasmic enzymes that would be released to the droplet environment upon cell lysis. The droplets can be either sorted or not sorted and then further analyzed for identification of tumor cell epitopes recognized by the t-cell.

Example 7

The present invention provides methods of matrix screening using a phased-drop approach or derivatives thereof. A device composed of a multitude of samples each separately contained within sample wells connected to one or more inlet channels such that that can be operated in such a way that each sample can be encapsulated within a droplet within a fluid-flow and be both sequentially and separately combined with each of the other samples by varying the phase of the combining of the separate, sequential droplets.

For example, by changing the phase of the combining of the drops it is possible to have, for example, with five separate samples each combine with the other samples, in this example in pairs, to yield drops containing a mixture of all possible pairs of compounds 1+2, 2+3, 3+4, 4+5, 5+1, . . . 1+4. The phasing can be by one of several means, including channel length, valves, pressure, etc.

In another example, a matrix of 100 chemical compounds are loaded into 100 separate wells and are each combined in separate pairs to yield 100^2 different pairwise combinations. These 10^3 combinations are each separately used in a cell-based assay to determine their combined effects on cell survival.

The devices and systems disclosed herein have several distinct advantages over current devices and methods for analyzing samples. These advantages include, for example: reliability and reproducibility, flexibility (the ability to 'swap out'), the greatly reduced cost of an assay, speed and handling, reduced skill-level required needed to perform the an analysis, scalability of assays from one to many nanoreactors, automatable with current liquid-handling robotics, multiple sort capability and previously unachievable assay architecture enabled by NanoRector confinement and manipulation

The enhanced functionality that electrostatic charge brings to droplets in microfluidic devices has the potential to enable an expansive list of microfluidics applications. This toolkit of techniques for manipulating droplets described herein can enable modular integration of systems for trans-

porting and reacting small numbers of molecules. High throughput screening, combinatorial chemistry, and the search for rare biological function in libraries of biomolecules all benefit from electrostatic manipulation of droplets in microchannels. Droplet-based microfluidic technology can also be used to develop a chip-scale fluorescence activated cell sorter (FACS) with enhanced activation functionality that goes beyond fluorescence to include multiple reagent-based assays between the droplet formation and sorting steps. Moreover by using femtoliter droplets, which are a few microns in diameter, even a single biomolecule represents concentrations of $\gg 1$ nM, sufficient for efficient chemical reactivity and single-molecule assays.

Many of the potential uses of droplet-based microfluidic devices are driven by a need to encapsulate a varied population or library of molecules, cells or particles into microreactors, perform an assay on the contents, perhaps through the addition of reagents, and then, finally, to selectively remove specific microreactors from the collection in a search for rare events. This requires a processing rates of 10³ per second to sort through the smallest libraries in a reasonable time while rates on the order 10⁵ per second are desirable for larger libraries. These rates are feasible using the charged droplet paradigm. Moreover, because the microfluidic devices are stamped, parallel flow streams can be fabricated, further enhancing the total throughput. Combined, the advantages of droplets and high throughput manipulation provide significant opportunity for widespread application. The inventions presented and described in detail herein will facilitate the application of droplet-based microfluidic technology.

Example 8

The present invention also provides adaptations of known assays for use on the microfluidic device according to the present invention. For example, fluorescence polarization, molecular beacons, and taqman assays can be adapted for use in SNP, DGE, and nucleic acid identification. In a high-throughput mode the individual droplets can be labeled with either organic or inorganic dyes, or colored beads. A distinct advantage is that beads are not required and the entire assay can be performed in solution. Some exemplary assays are described.

The present invention can be used to identify CDRs in a pre-defined CDR library. In one example, there can be 100 pre-defined CDRs for each of the 6 CDRs in an scFv (i.e., 3 in VH, and 3 in VL). 600 molecular beacons can be created, each beacon separately emulsified with a different (for example, q-dot) LiquidLabel. The 600 separate emulsions can be pooled to create one emulsion library mixture (composed of 600 different types of droplets, and as stated each droplet containing both a molecular beacon specific to a specific CDR, and a LiquidLabel specific to droplets containing that molecular beacon). scFv Ab genes from antigen-interacting antibodies isolated by either phage display or yeast two-hybrid can be amplified by PCR using 5' and 3' flanking primers. The PCR product of the Ab gene can be either emulsified on the RDT Instrument prior to combining with the library mixture, or, in a separate example, combined with its own unique LiquidLabel off-line, and mixed with several (other) amplified Ab fragments, thereby allowing several PCR fragments to be analyzed simultaneously. The amplified fragment will then be combined with the library mixture, and run past the detector. The detector will identify the molecular beacon within the droplet using the LiquidLabel and further detect whether hybridization has

occurred by examining the status of the fluorophore relative to the probe-containing quencher.

An oligonucleotide assay can be used to generate a product against which an fluorescence polarization (FP) organic-dye type tag, molecular beacon or taqman oligonucleotide can be used in an assay as described above. Other assays are also possible.

The present invention can also be utilized in differential gene expression. Taqman or molecular beacons can be used in a modification of the methods as described herein.

The TaqMan system requires the use of a polymerase with 5' to 3' nuclease activity, such as Taq DNA polymerase, and a short oligonucleotide probe labeled with a reporter dye and a quencher dye that anneals to the target downstream from one of the primers (See, FIG. 12, left panel). If the probe is hybridized to the target, the polymerase cleaves the hybridized probe, separating the reporter from the quencher, which results in a higher fluorescent signal. The fluorescent signal increases proportionally to the number of amplicons generated during the log-linear phase of amplification. It is important that the probe hybridizes before the primers so the polymerase can cleave the probe and release the reporter dye as primers are extended. Otherwise, amplification occurs but is not monitored because the probe is not cleaved.

Molecular beacon probes are hairpin-shaped oligonucleotide molecules that have a fluorophore and a non-fluorescent quencher dye attached to the 5' and 3' ends (See, FIG. 12, right panel). Generally, DABCYL is the non-fluorescent universal quencher and the other dye is a reporter fluorophore such as, FAM, TET, TAMRA or ROX. The molecular beacon is in a hairpin configuration when it is not hybridized to the target site. It is designed to have two "arms" with complementary sequences that form a very stable hybrid or stem. The close proximity of the quencher and reporter suppresses reporter fluorescence when the beacon is in a hairpin configuration. When the beacon hybridizes to the target during the annealing step the reporter dye is separated from the quencher, which allows the reporter to fluoresce. In order for the beacon to anneal to the target sequence, it must form a hybrid that is even more stable than the hairpin to remain in the hybridized conformation. Therefore, the probe is less likely to form a hybrid with the target if there are mismatched base pairs.

In addition to molecular beacons and Taqman, the devices of the present invention can be used to carry out fluorescence polarization as described herein. Most SNP assays can be adapted for both mini-sequencing and gene expression analysis. A series of fluorescence polarization measurements have been made inside a microfluidic device according to the present invention while looking at droplets containing Fluorescein, Fluorescein bound to biotin, and Fluorescein bound to biotin+Streptavidin. The fluorescence signal was split into two orthogonal polarizations: one parallel to the laser excitation polarization, and one perpendicular to the polarization. These signal were collected and analyzed to determine the change in polarization of the fluorescence for each of these binding conditions.

The Polarization is calculated from:

$$P = \frac{(V - H)}{(V + H)}$$

Where V=fluorescence signal polarized parallel to laser excitation polarization, and H=fluorescence signal polarized perpendicular. A mP ("milli-P") is 1000*P. The Polarization

is equal to zero when the fluorescence is completely depolarized, and has a maximum of 500 mP when the fluorescent molecule is “frozen” (i.e. bound to a large molecule that does not rotate between excitation and emission).

The fluorescence station was modified to include cleanup polarizer for the laser and a polarizing beamsplitter with cleanup polarizers for collection. The two resulting fluorescence channels collect light with orthogonal polarizations (“Vertical” is parallel to the laser polarization, “Horizontal” is perpendicular to the laser polarization). The device used to generate alternating droplets is built from RDT Master #257 (50 um deep channels). Table 2 lists the fluids used for these tests.

TABLE 2

Fluids ran through the double nozzle device.	
Fluid name	Composition
Oil	FC3283 + 10% “Avocado”
BTFC	1×10^{-6} Molar Biotinylated Fluorescein in 10 mM Borate pH 9
BTFC + SA	1×10^{-6} Molar Biotinylated Fluorescein in 10 mM Borate pH 9 + 0.5×10^{-6} Molar Steptavidin (4 binding sites per molecule)

During these experiments, the fluid flow rates were 200 ul/hr for FC, BTFC, and BTFC+SA, and 600 ul/hr for the oil (FC3283+10% “Avocado”). Droplets ranged in size from 65 to 75 um in diameter, depending on which water solution was used. Time between droplets varied from 1300 us to 2200 us, again depending on which fluid was used. Fluorescence polarization measurements were made by injecting BTFC in one nozzle, and BTFC+SA in the other. Once these measurements were completed, the BTFC+SA was replaced with FC and a second series of data was collected. FIG. 13 plots typical fluorescence data collected from both these runs, as well as the calculated Polarization for each of the droplets shown. FIG. 13 (top panel) shows raw polarized fluorescence signals collected on the test station when measuring BTFC and BTFC+SA, then BTFC and FC (the data is normalized so $P(\text{Fluorescein})=0.0$). FIG. 13 (bottom panel) shows polarization calculated from each droplet in the top plot. The transition at $t=1.5$ sec is a mathematical artifact where the data collected for the two conditions were concatenated in software (the data after $t=1.5$ was collected approximately 30 minutes after the data collected before $t=1.5$). In this data, Vertical is fluorescence parallel to laser polarization, Horizontal is polarization perpendicular. In this data, the “horizontal” polarization has been normalized such that the Polarization is equal to zero for Fluorescein. The Polarization was calculated by integrating the fluorescence signal across the droplet for each polarization, then plugging the results into Equation 1. FIG. 14 plots the Polarization measured for a longer number of droplets, along with the histogram created from this data. FIG. 14 (top panel) shows polarization calculated from each droplet for a longer time period than in FIG. 3. FIG. 14 (bottom panel) shows histogram generated from the data in the top figure. The data after $t=1.5$ was collected approximately 30 minutes after the data collected before $t=1.5$.

As seen in the histograms of the Polarization, the polarization clusters tightly around three different mean values. The zero-centered mean ($\sigma=1.7$) corresponds to Fluorescein, while the 18.4 mP ($\sigma=1.6$) grouping corresponds to Biotinylated Fluorescein and the 96 mP ($\sigma=3.46$) grouping corresponds to Biotinylated Fluorescein bound to Steptavidin.

Example 9

Fluorosurfactants are synthesized by reacting Krytox 157 FSL, FSM, or FSH with aqueous ammonium hydroxide in a volatile fluorinated solvent. The solvent and residual water and ammonia are removed with a rotary evaporator. The surfactant can then be dissolved in a fluorinated oil (e.g., FC-3283 from 3M), which can then be used as the continuous phase of the emulsion. A typical concentration is 2.5 wt % of surfactant dissolved in the oil.

The channels of the microfluidic device are also coated with a fluorinated surface product. For example, the coating is applied from a 0.1-0.5 wt % solution of Cytop CTL-809M in CT-SoIv 180. This solution is injected into the channels of a microfluidic device via a plastic syringe. The device is then heated to 90° C. for two hours, followed by 200° C. for an additional two hours. These surfactants in the fluorinated oil stabilize the aqueous droplets from spontaneously coalescing. By fluorinating the channel surfaces, the oil phase preferentially wets the channels and allows for the stable generation and movement of droplets through the device, the low surface tension of the channel walls minimizes the accumulation of channel clogging particulates.

Example 10

The quality of libraries of emulsified compounds can also be controlled so as to eliminate from the library those compounds that cross between droplets. By emulsifying a q-dot encoded, buffer-only droplet and allowing it to incubate with 1-1000 separately emulsified compounds quality control of libraries can be achieved. After incubation, the uniquely encoded q-dot droplet is sorted away from the compound-containing droplets and analyzed (e.g., by mass spec) for the presence of any of the compounds emulsified in the other 1-1000 types of droplets. Compounds that cross between droplets are identified and eliminated from the library.

Example 11

The present invention also enables the user to sort cells based on binding of an affinity-reagent attached to a means for signal amplification. As a non-limiting example, an antibody fused to an enzyme (e.g., alk/phos, β -gal, horseradish peroxidase, etc.) is added to a mix of cells and incubated. The antibody can be against a particular cell-surface marker, for example, such as a cancer marker. The cell suspension can be washed or unwashed (if the antibody is in low concentration, i.e., less than 1 antibody per droplet, and the antibody has good binding properties).

The cells that have antibodies attached to them are then emulsified into droplets and an appropriate enzyme-substrate is added. The presence of a fluorogenic substrate product is amplified from one to many copies by the enzyme turning-over the substrate. Multiple enzymes and multiple substrates can be used to allow analysis of multiple samples with multiple fluorophores at the same time or sequentially. The affinity-reagent can be a protein, nucleic acid, or other molecule to which an enzyme (or portion thereof that when brought together becomes active) can be attached either covalently or through a reasonably strong interaction.

Example 12

The device of the present invention can also be used to sequence individual exons from individual chromosomes or

tumor cells. A schematic diagram for performing this method is provided in FIG. 19. Individual specific primer-pairs to different exons (e.g., epidermal growth factor receptor (EGFR) exon-specific primer pairs) along with a primer-bound bead (e.g., a Dynal streptavidin bead) are each emulsified and then pooled to create a library emulsion (in FIG. 19 a set of 96 exon primer pairs are shown for illustrative purposes). Separately, a chromosomal DNA solution is diluted in an aqueous buffer such that upon emulsification on a microfluidic device described herein, a 30-50 micron droplet contains, on average, slightly less than a half-genome's concentration of DNA. Droplets from the pooled emulsion library set of exon-specific primers are coalesced with droplets containing the diluted solution of chromosomal DNA on a microfluidic device as described herein, and used in a bead-based DNA amplification reaction (i.e., PCR). The microfluidic device as described herein collects 1×10^9 of these droplets in 24 hours, which results in an emulsion of droplets, some of which contain beads with amplified exon-DNA attached. After PCR, the emulsions are broken by centrifugation, the beads are isolated, washed, and then enriched for DNA-containing beads on a microfluidic device as described herein. The exon- and chromosome-specific DNA-containing beads are randomly placed into a picotiter plate (454 Corp.) and sequenced using a Life Sciences DNA sequencing instrument (as provided by 454 Corp. and described in any of U.S. application Ser. No. 09/814,338, filed Mar. 21, 2001; U.S. application Ser. No. 10/104,280, filed Mar. 21, 2002; U.S. application Ser. No. 10/767,899, filed Jan. 28, 2004; U.S. application Ser. No. 11/045,678, filed Jan. 28, 2005; or U.S. application Ser. No. 11/195,254, filed Aug. 1, 2005, each of which are incorporated herein by reference in their entirety). A summary of this process is provided by FIG. 20. The emulsion PCR amplification reaction can be performed off-chip using control chromosomal DNA as template and a single set of exon-specific primers, or on-chip (i.e., on the microfluidic devices of the present invention as described herein).

In a more specific example, the microfluidic devices and methods of the present invention have been used to develop individual exon-, and chromosome-specific sequencing methods with off-line emulsion PCR using chromosomal DNA as template and a single set of exon-specific primers.

The ability to combine (i.e., coalesce) two droplets together can be used to amplify an exon from an individual chromosome.

a. PCR Amplification of DNA within a Droplet.

454 Life Sciences has previously demonstrated emulsion solid-phase PCR in droplets of a size range anticipated for the microfluidic devices according to the present invention. Successful DNA amplification using an emulsion of a PCR with the perfluorocarbon oils and surfactants used to generate and manipulate droplets on microfluidic devices of the present invention have also been demonstrated. Several polymerases (notably those from archea, e.g., Thermal Ace DNA Pol; Pfu Turbo Pol; Advantage 2-CG Taq Pol; and Advantage Taq Pol) work well in the buffers and oils used in the devices described herein.

b. Setting Up the Exon-Specific PCR Reactions.

In the first set of experiments, robust bulk conditions for the droplet-based exon amplification are developed. Primers within an exon in the EGFR gene can be used. Approximately 10% of patients with non-small-cell lung cancer (NSCLC) show responsiveness to targeted tyrosine kinase inhibitor (TKI) chemotherapy regimens. Response in patients has been strongly associated with somatic heterozygous mutations in the ATP cleft of the EGFR gene.

Wild-type and mutant chromosomal DNAs containing an 18 base pair (bp) deletion in an EGFR exon encoding this ATP cleft are used. Initial experiments can be performed in a bulk (i.e., off-instrument) solution using the perfluorocarbon oils and surfactants as described herein. Once conditions have been established with limiting chromosomal DNA these amplification experiments in mono-dispersed droplets formulated on-instrument are repeated. These droplets are collected and the DNA contained within amplified. The emulsion containing the amplified droplets are broken, and the aqueous phase analyzed by gel electrophoresis.

c. Measurement of Solid Phase Amplification.

Once the exon PCR reactions are working in solution from droplets formed on the instrument, these experiments will be repeated with droplets containing both primers and beads. The beads are emulsified with the exon primer pairs. One of the primers is attached to the bead using standard oligonucleotide coupling chemistry. Both primers will also be in solution (those skilled in the art will appreciate that the goal of solid-phase amplification is to generate enough amplified product in solution such that some of it is driven to the oligonucleotide primer attached to the bead). A serial dilution of chromosomal DNA in several trials is then added to the primer-bead solution. Droplets are formulated at a concentration of less than one bead per droplet. The DNA/primer/bead solution is gently shaken to keep the beads in suspension as the droplets are being formed on the microfluidic devices of the present invention. The droplets are collected from the instrument and the DNA within them is amplified by PCR off-line.

d. Measurement of Single-Chromosome PCR.

On-bead hybridization of two separately-labeled cy3- and cy 5-containing oligonucleotide probes is used to measure amplified-DNA attachment efficiency. A cy3-labeled probe is synthesized complementary to the sequence within the 18 bp deletion region, and a second cy5-labeled oligonucleotide probe is synthesized that will span this deletion (with complementarity to both 5' and 3' sides). The probes are designed such that at 30° C. they do not cross-hybridize. The quantitation and ratio of cy3:cy5 dyes on the bead is a measure of the amount of each specific allele of the DNA present on the bead.

As a control, a fluorescein-labeled oligonucleotide complementary to the oligonucleotide attached to the bead is used. This control oligonucleotide is used to estimate the maximum amount of cy3 or cy5-labeled probe that can attach to the bead. The hybridized beads are washed to remove un-hybridized probe and the amount of fluorescein still attached to individual beads is compared to fluorescein-standard concentrations. Other methods and controls for estimating attached DNA (such as fluorescence polarization) can be used in conjunction with the microfluidic devices according to the present invention. FIG. 21. The chromosomal DNAs are diluted and added to exon-primer containing droplets on the microfluidic devices of the present invention using conditions established in the bulk emulsions. After PCR amplification, the beads are isolated, washed, and hybridized in solution to the cy3-, cy5-labeled probes. The hybridized beads are washed to remove un-hybridized and non-specifically-bound labeled nucleotide and the amount of dye still attached to individual beads is determined using a fluorescent microscope. The % synthesized is estimated from the maximum estimated to be able to be synthesized. The 454 instrument requires 1×10^7 copies of DNA per bead for accurate reads. Using the methods described herein, more than 1×10^7 DNA molecules per bead can be attached.

PCR is a typical temperature-controlled and enzyme catalyzed biochemical reaction that consists of the periodical repetition of three different temperatures (melting, annealing and extension temperature). Alternatively, two temperatures can be applied by combining the annealing and extension temperatures, thus further reducing the complexity of the thermal cycling profile and increasing the speed and efficiency of the PCR reaction. Because of the temperature-sensitivity of the PCR system a minor temperature difference may significantly affect the efficiency of DNA amplification, especially in emulsion PCR microfluidic systems.

Accordingly, the effects of temperature on enzyme kinetics, heating and temperature-measuring methods in emulsion PCR microfluidics are critical in order to gain a better understanding of PCR kinetics in microfluidics.

Several thermostable polymerases that work well in oils used in the microfluidic devices have been identified herein. A syringe pump attached to a microfluidic device of the present invention with appropriate sensors and heating elements (described below) can be used to model the ability of the polymerases to generate PCR product off-instrument.

The choice of a heating method for PCR microfluidics is of importance for achieving faster temperature ramping rates. In one embodiment, a contact-heating method (e.g., the use of hot air) can be used. Contact-heating methods utilize electrothermal conversion to heat the PCR solution, in which the thermal components embedding the heating element are in direct contact with the components of the PCR amplification. To date, along with the thin film heaters, metallic heating blocks and Peltier-effect-based thermoelectric ceramic heating blocks have been widely applied in temperature control of PCR.

In one embodiment, 2 Kaptan Thermofoil heaters from Minco and a two-step PCR cycling method can be used. Thermofoil heaters are thin, flexible heating elements consisting of an etched foil resistive element laminated between layers of flexible insulation. Thermofoil heaters are applied to the surface of the part to be heated. Their thin profile gives close thermal coupling between the heater and heat sink. The flat foil element of thermofoil heaters transfers heat more efficiently and over a larger surface area than round wire. Thermofoil heaters, therefore, develop less thermal gradient between the resistive element and heat sink.

Methods of Temperature Measurement for PCR Microfluidics.

In emulsion PCR microfluidics, it is critical to select methods for temperature measurement to accurately control temperature during PCR cycling. Temperature measurement methods are usually divided into two categories: contact and non-contact temperature measurement. The former includes thin-film type temperature sensing and non-thin-film-type temperature sensing.

In one embodiment, temperature measurement can be performed by using the Minco Non-Invasive Sensors Design Kit. This kit comes with thermal-ribbon, thermal-tab, and bolt-on resistance temperature detectors that will allow us to accurately sense temperature without having to drill or tap into the chip. The detectors are accurate to $\pm 0.25^\circ$ C. In another embodiment, temperature measurements using a temperature dependent fluorescent dye (e.g., a dilute fluorophore such as rhodamine Borrhodamine 3B) can constitute a second technique for measuring temperature in microfluidic structures.

The methods discussed above can be repeated with a second primer set, which consists of 96 different exons. Primers can be designed and tested on an MJ Research PCR instrument a priori to establish suitability to the two-step PCR conditions to be used on-chip.

All exons to be amplified are first sequenced by traditional Sanger methods to establish a base-line read. Where possible, exons with known polymorphisms within the to-be-sequenced DNA (i.e., the individual will be polymorphic at a site within the exon) are selected. We expect 50:50 for each polymorphism, this analysis will enable us to gather information about the bias in sequencing during the on-chip amplification reactions. The controls for attachment are the same as that described above.

A pool of primer sets are tested on a diluted genomic DNA solution whereby the genomic DNA is at several concentrations.

Once the ideal amount and quality of DNA attached to the beads is achieved, the 454 instrument will be used to sequence the beads. DNA-containing beads are enriched for on microfluidic devices according to the present invention either using a DNA staining agent (ex, Syber green) or by hybridization to a fluorescent oligonucleotide probe. Appropriate controls are used to estimate the number of exon copies per bead.

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33

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What is claimed is:

1. A method for detecting a target nucleic acid fragment from a sample, the method comprising:

providing a sample comprising a plurality of different nucleic acid fragments;

partitioning the sample into a plurality of droplets, wherein each of the plurality of droplets comprises one or more of the different nucleic acid fragments, reagents for an amplification reaction, and one or more different optically labeled probes specific for one or more different nucleic acid fragments;

amplifying the different nucleic acid fragments in a plurality of droplets;

flowing the plurality of droplets comprising the different amplified nucleic acid fragments past a detector that detects polarized light;

detecting a level of polarized light emitted from each of the plurality of droplets

comprising the different amplified nucleic acid fragments as each of the plurality of droplets flows past the detector;

comparing the detected polarized light emitted from each of the plurality of droplets, comprising the different amplified nucleic acid fragments from the different portions of the sample in each of the plurality of droplets, to one another; and

identifying the different amplified nucleic acid fragments from the different portions of the sample in one or more of the plurality of droplets in order to detect the different amplified nucleic acid fragments.

2. The method of claim 1, wherein a high level of polarized light is indicative of an absence of the target nucleic acid fragment.

3. The method of claim 1, wherein a low level of polarized light is indicative of a positive presence of the target nucleic acid fragment.

4. The method of claim 1, wherein the one or more different optically labeled probes each comprise a fluorescent label.

5. The method of claim 1, wherein the one or more different optically labeled probes each further comprise a quencher molecule.

6. The method claim 1, wherein the probe further comprises a moiety that alters polarization of light emitted from each of the plurality of droplets.

7. The method of claim 1, wherein the sample is a human tissue or body fluid.

8. The method of claim 1, wherein each of the plurality of droplets comprises one nucleic acid fragment.

9. A method for detecting a target nucleic acid from a sample, the method comprising:

providing a sample comprising a plurality of different nucleic acid fragments;

partitioning the sample into a plurality of droplets, wherein each of the plurality of droplets comprises one or more of the different nucleic acid fragments, reagents for an amplification reaction, and one or more different detectably labeled probes specific for one or more different nucleic acid fragments;

amplifying the different nucleic acid fragments in a plurality of droplets;

configuring a polarization filter with respect to an excitation polarization;

flowing the plurality of droplets comprising the different amplified nucleic acid fragments past a detector that comprises the polarization filter;

detecting a level of polarization light emitted from each of the plurality of droplets comprising the different amplified nucleic acid fragments as each of the plurality of droplets flows past the detector;

comparing the detected polarized light emitted from each of the plurality of droplets, comprising the different amplified nucleic acid fragments from the different portions of the sample in each of the plurality of droplets, to one another; and

identifying the different amplified nucleic acid fragments from the different portions of the sample in one or more of the plurality of droplets in order to detect the different amplified nucleic acid fragments.

10. The method of claim 9, wherein the detectable label is a fluorescent label.

11. The method of claim 10, wherein the detector is configured such that the polarization filter is perpendicular to the excitation polarization.

12. The method of claim 11, wherein a high level of polarized light is indicative of an absence of the target nucleic acid fragment.

13. The method of claim 11, wherein a low level of polarized light is indicative of a positive presence of the target nucleic acid fragment.

14. The method of claim 9, wherein the probe further comprises a quencher molecule.

15. The method claim 9, wherein the plurality of droplets each comprise one nucleic acid fragment.

16. The method of claim 10, wherein the detector is 5 configured such that the polarization filter is parallel to the excitation polarization.

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