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(54) **MEDICAL DEVICE AND PROCEDURE
SIMULATION**

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G09B 23/30 (2006.01)

(52) **U.S. Cl.**
CPC **G09B 23/30** (2013.01)

(58) **Field of Classification Search**
CPC G09G 23/28; G09G 23/30; G09G 23/285; G09G 23/288
USPC 434/272, 262
See application file for complete search history.

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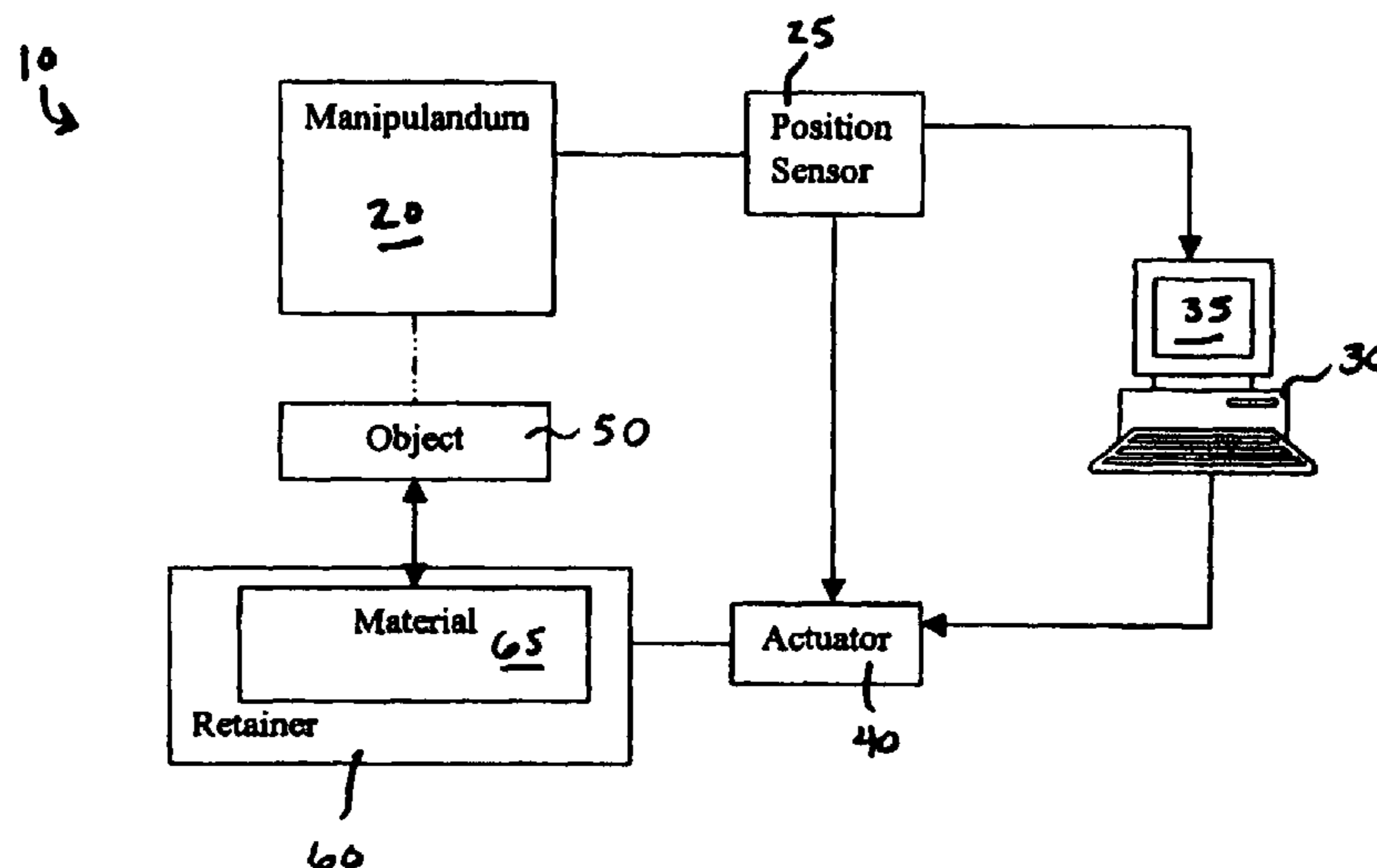
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(57) **ABSTRACT**

A device is disclosed that includes an interface member including a material and a manipulandum movable in a degree of freedom. The manipulandum is able to penetrate the material. A sensor is configured to output a position signal based on the position of the manipulandum. An actuator is configured to output haptic feedback by applying a compressive force to the material based on the position signal. In other embodiments, a method is disclosed that includes receiving a position signal associated with a position of a manipulandum, where at least a portion of the manipulandum penetrates the interface material. Haptic feedback is output by varying a density of the interface material based on the position signal.

22 Claims, 6 Drawing Sheets



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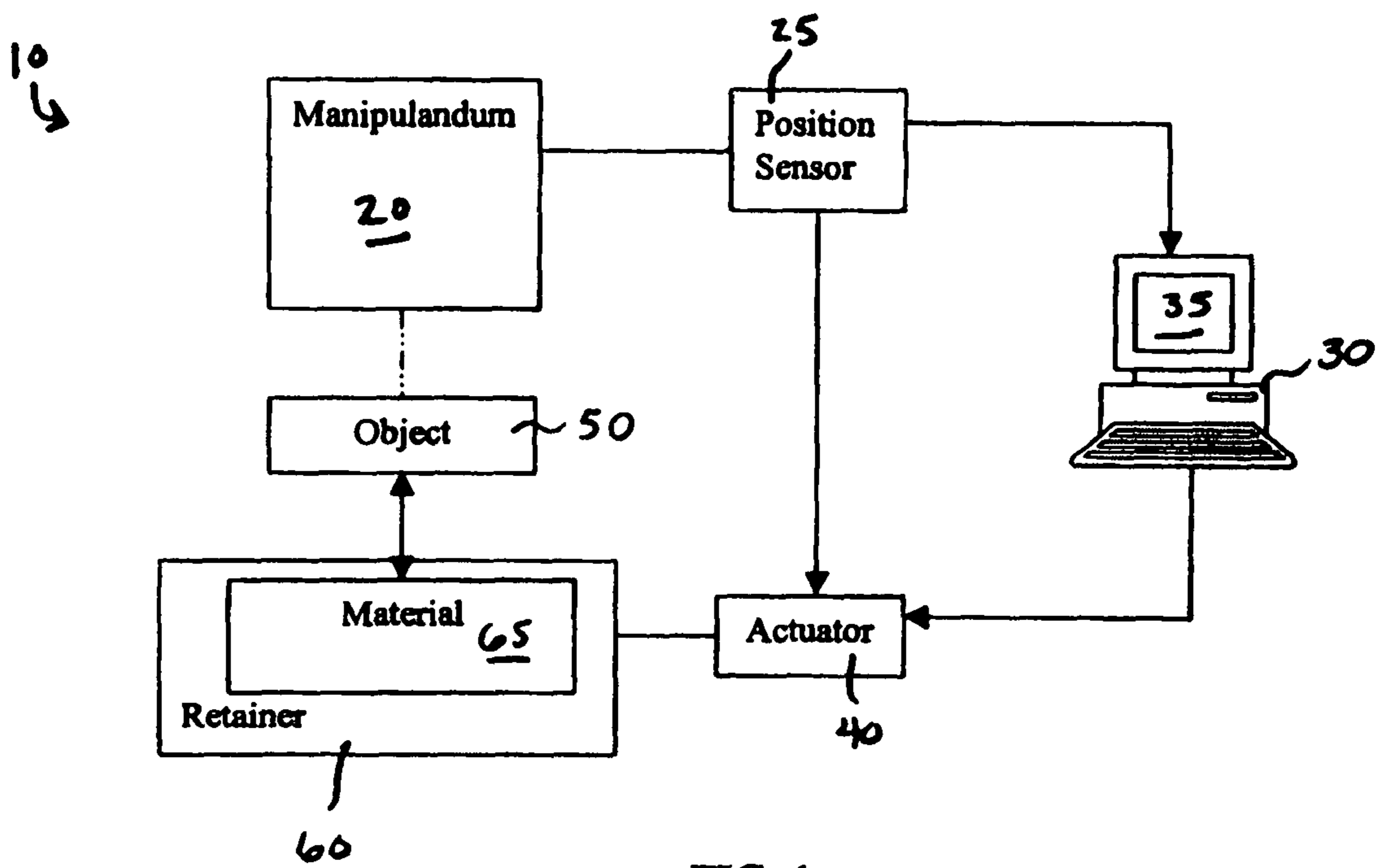


FIG. 1

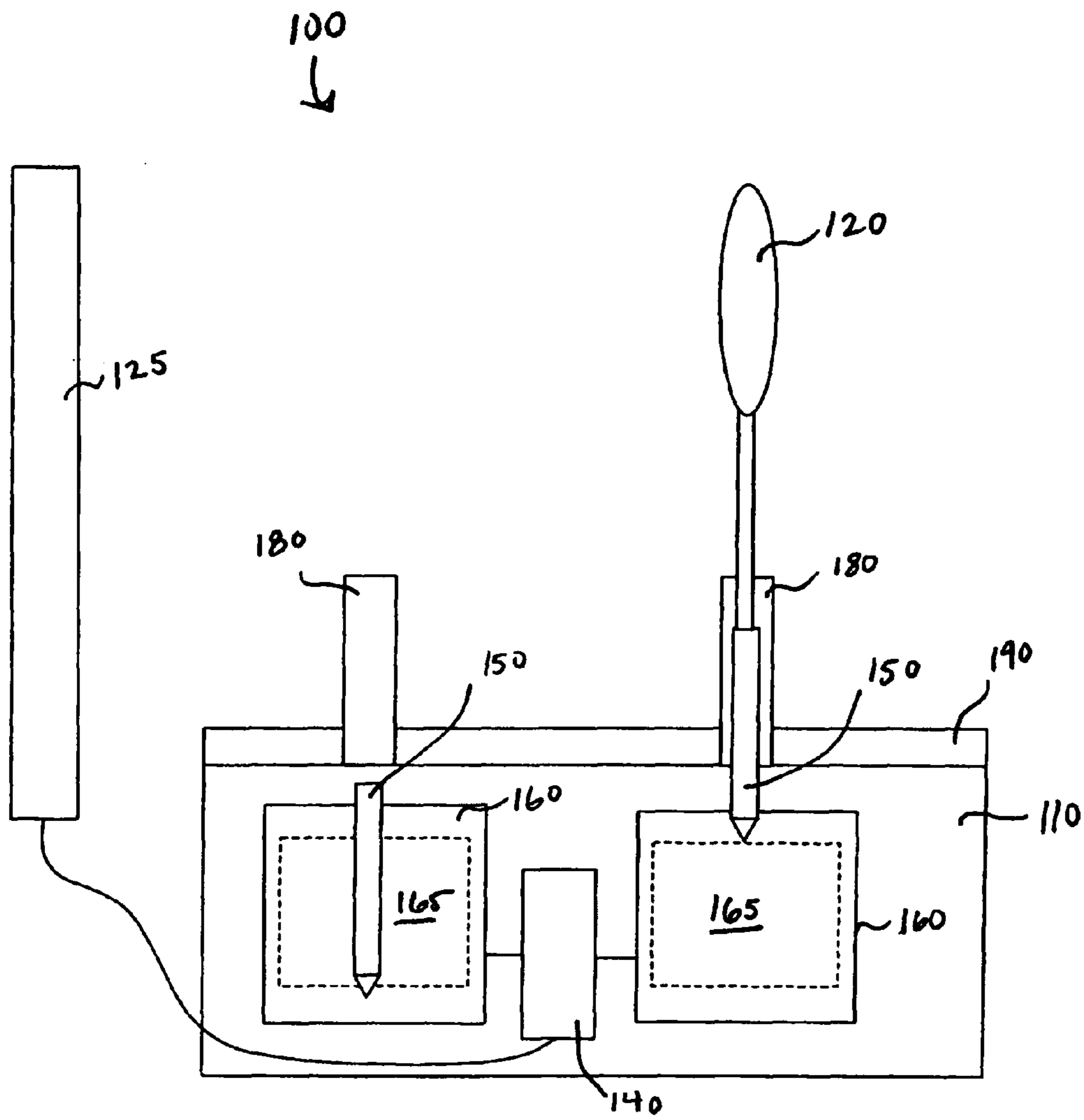
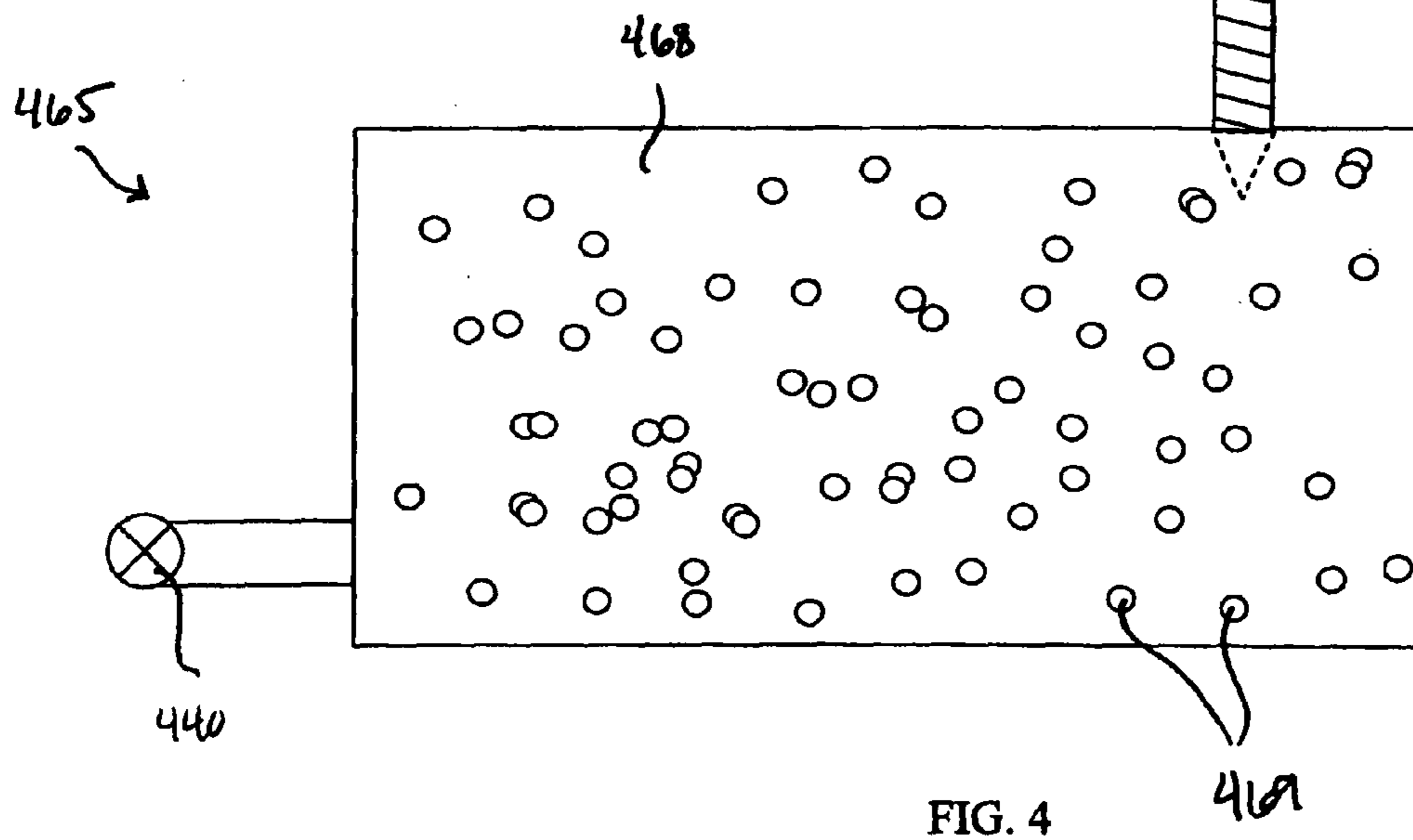
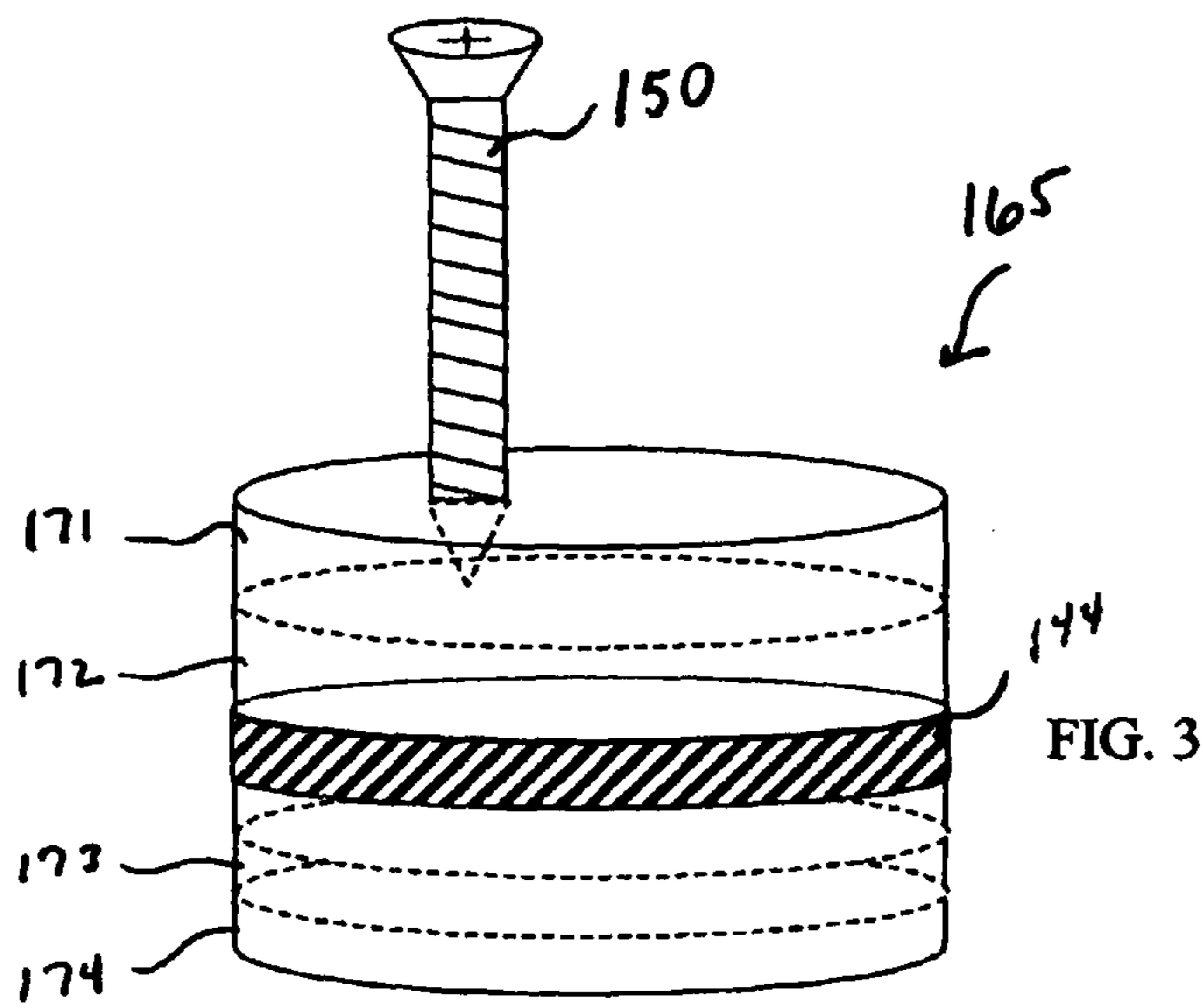


FIG. 2



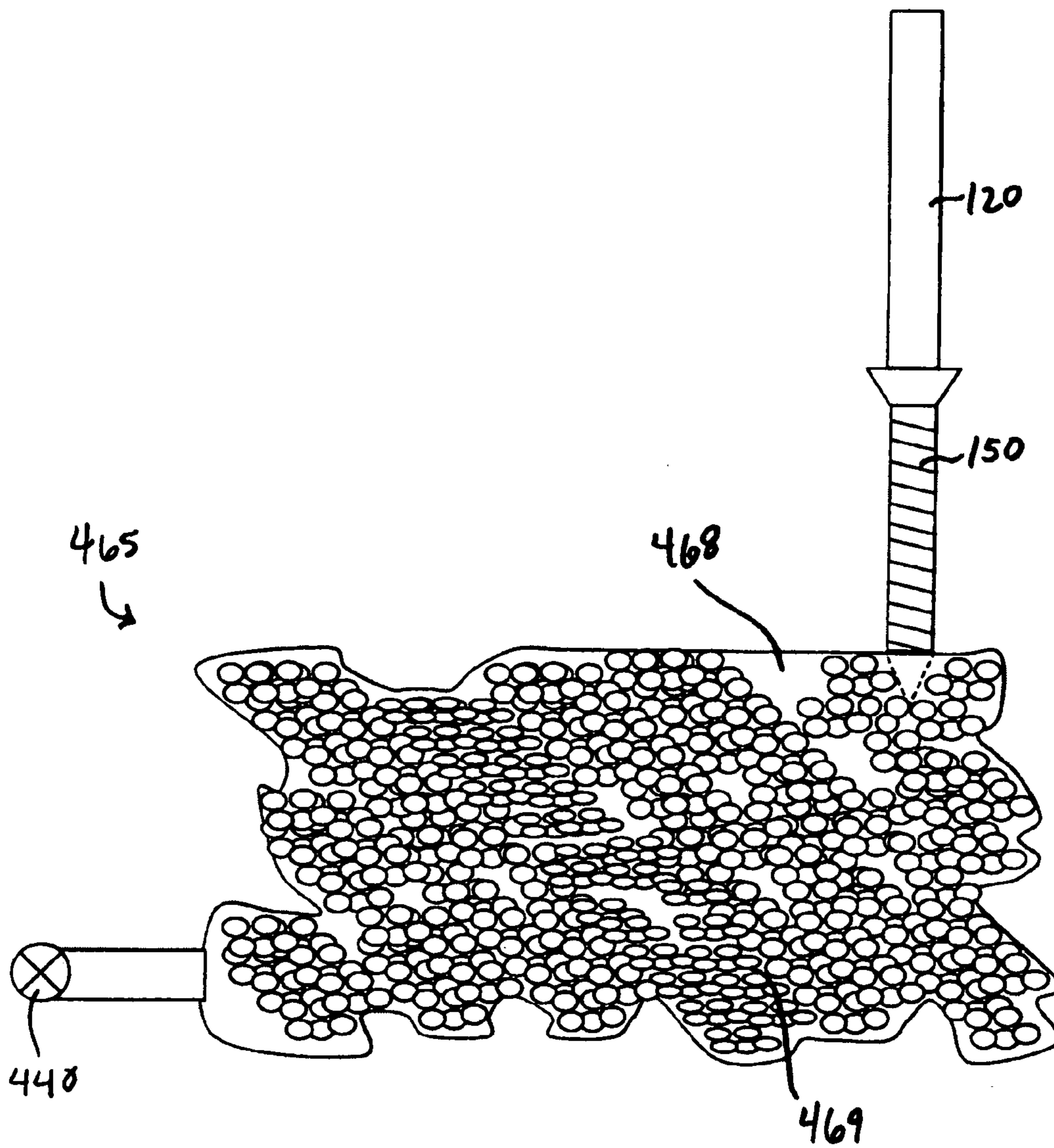


FIG. 5

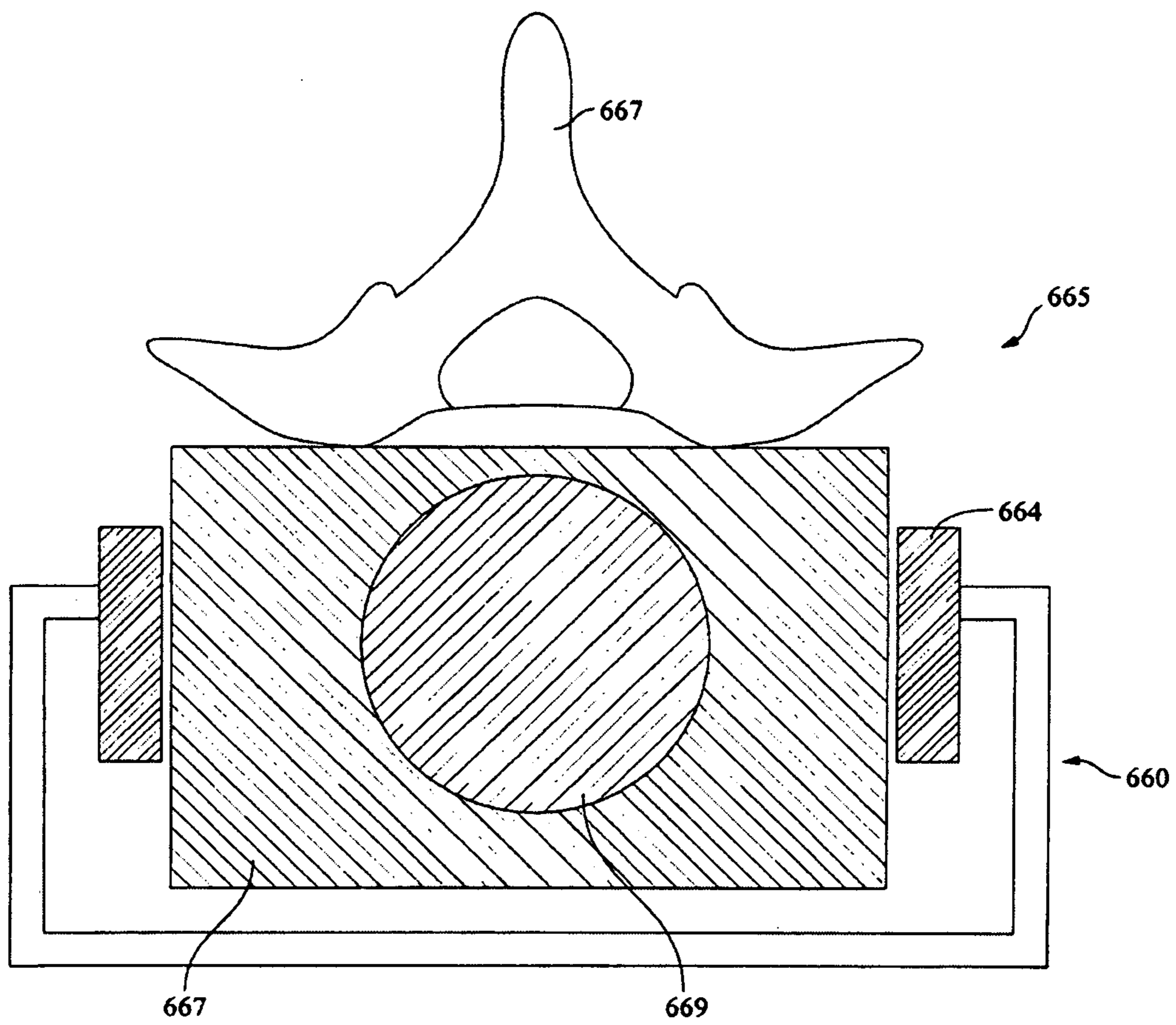


FIG. 6

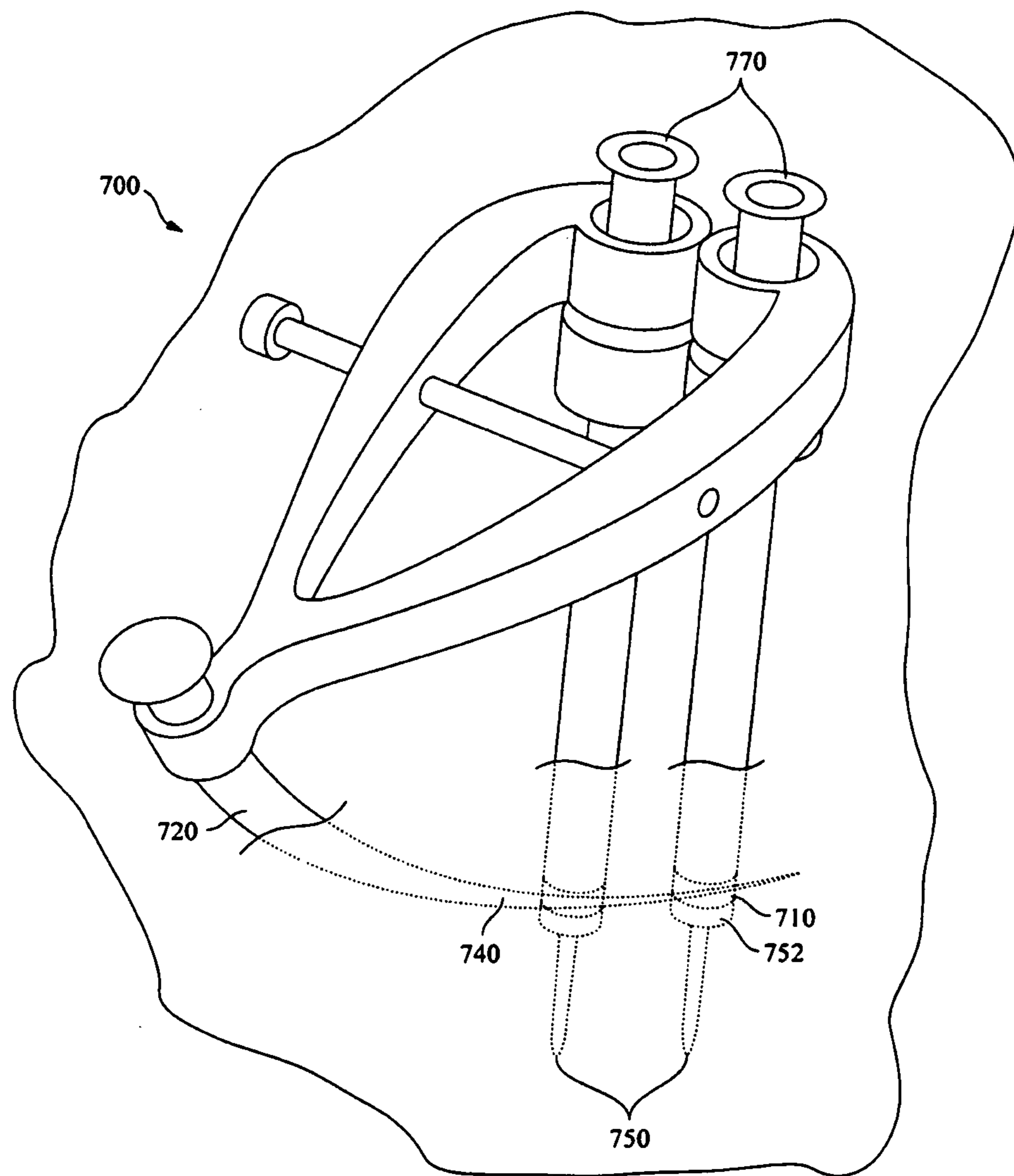


FIG. 7

MEDICAL DEVICE AND PROCEDURE SIMULATION

CROSS-REFERENCE TO RELATED APPLICATIONS

The present application is a continuation of co-pending U.S. patent application Ser. No. 10/803,080 filed Mar. 18, 2004, in the name of inventors Richard L. Cunningham and Robert Cohen and entitled "Medical Device and Procedure Simulation", commonly owned herewith.

BACKGROUND

The invention relates generally to medical procedure simulations, and more particularly to a method and apparatus for simulating a spinal stabilization procedure.

Minimally invasive medical procedures reduce danger to patients, decrease recovery time, and provide superior outcomes when compared to open surgery. The physician typically operates at a distance from the surgical site, however, frequently using remote cameras or other imaging modalities, and remotely controlled surgical tools. Consequently, these procedures can be difficult to master. Thus, the use of procedure simulation systems provides a learning environment in which the physician can gain needed skills without putting patients at risk.

A known minimally invasive spinal stabilization procedure uses four screws and two connecting rods to stabilize two adjacent vertebrae. The procedure makes six puncture incisions; one each for the four screws and the two connecting rods. After two screws are inserted in adjacent vertebrae, they are connected with a curved rod and the procedure is repeated with two more screws. The connecting rod is aligned with slots in two screws by means of a device that constrains the curved rod to move in an arc that is constrained to properly align the two screws, which are in turn each attached to two legs of the alignment device.

Known medical procedure simulators have been developed that simulate the functionality of open spinal procedures. In one example of such simulators, a user manipulates various devices in connection with simulated bone structure. The bone structure is simulated with castings fabricated from a material such as compressed sawdust. Minimally invasive procedures, however, use fluoroscopic guidance systems. A simulator using such technology would be expensive to produce and would needlessly expose the user to radiation. Additionally, using known physical model simulation techniques would not allow the simulation of certain features such as physical anatomical variations (e.g., varying bone densities), vital signs and other important aspects of the procedure.

Thus, a need exists for a medical procedure simulation device and method that can combine physical models with computer controlled feedback, simulated fluoroscopy, and simulated physical anatomical variations to enable the user to experience a more realistic training experience.

Overview

A device is disclosed that includes an interface member including a material and a manipulandum movable in a degree of freedom. The manipulandum is able to penetrate the material of the interface member. A sensor is configured to output a position signal based on the position of the manipulandum. An actuator is configured to output haptic feedback by applying a compressive force to the material based on the position signal.

In other embodiments, a method is disclosed that includes receiving a position signal associated with a position of a manipulandum, where at least a portion of the manipulandum penetrates the interface material. Haptic feedback is output by varying a density of the interface material based on the position signal.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic representation of a medical procedure simulation device according to an embodiment.

FIG. 2 is a block diagram of a device according to an embodiment.

FIG. 3 is a perspective view of an interface member for use with the device illustrated in FIG. 2.

FIG. 4 is a plan view of an interface member for use with the device according to an alternative embodiment under a first set of conditions.

FIG. 5 is a plan view of the interface member illustrated in FIG. 3 under a second set of conditions.

FIG. 6 is a cross-sectional view of a device according to another embodiment.

FIG. 7 is a perspective view of an example of a medical device that can be simulated by embodiments.

DETAILED DESCRIPTION

Devices and methods for simulating medical procedures are described. More specifically, a particular medical device for minimally invasive spinal stabilization and an associated procedure is described and then a simulation device and method for this medical device and procedure is described. The Medtronic Sofamor Danek CD HORIZON® SEXTANT™ Percutaneous Rod Insertion Set **700**, illustrated in FIG. 7, uses CD HORIZON® M8 cannulated titanium Multi-Axial Screws **750**. Cannulated screws **750** are used to facilitate percutaneous navigation of the pedicles of a vertebrae with a guide wire (not shown). A series of tubular dilators **770** are used to create a tunnel through the soft-tissues of the back, prior to placement of the screws **750** over the guide wire. The cannulated screws **750** are comparable in strength, profile, and fatigue resistance to the CD Horizon M8 multi-axial screws that are well known to spine surgeons. The screws vary in length from 35 to 55 mm long.

The rods **740** that are used to connect the pedicle screws are pre-cut and pre-bent in 5 mm increments for single level cases, and in 1 cm increments for bi-level cases. The pre-contoured rods range in size from 30 to 90 mm in length. The rods **740** are pre-contoured because the insertion technique depends upon a precise geometric arrangement of the screw heads **752** that are then matched to the radius of curvature of the rod **740**.

Each cannulated screw **750** is fitted with a specially designed screw extender **710** that allows the multi-axial heads to be manipulated independently. This extender **710** also has an integrated mechanism (not shown) for holding, engaging, and securing the setscrew (not shown) that fixes the rod **740** to the screw head **752**.

After the pedicle screws **750** have been inserted into the proper vertebral bodies (not shown) and their positions have been confirmed radiographically, the heads **752** of the pedicle screws **750** are connected to each other with rod **740**. The screw heads **752** can be percutaneously manipulated with the screw extenders **710**, and smooth rod insertion is made possible by connecting the two screw extenders **710** together, which assures that the multi-axial screw heads **752** are aligned along the same curvilinear path as the pre-contoured

rod 740. The geometry of the screw extenders 710 and rod introducer 720 dictates that the rod 740 follows a precise path, through the soft tissues and into properly aligned screw heads 752.

Proper torque on the setscrews (not shown) that secure the rod 740 to the pedicle screws 750 is assured with a “break-off” mechanism that snaps off the screw head when the proper torque has been reached. After the pedicle screw 750 and rod 740 construct has been assembled and confirmed with the fluoroscope, the setscrews are secured and torqued with the “break-off” mechanism. The device 700 can be simulated using embodiments of the invention as described below.

FIG. 1 is a schematic representation of a medical procedure simulation device 10 according to an embodiment of the invention. The device 10 includes a manipulandum 20 that is coupled to a position sensor 25 and is movable in at least two degrees of freedom. The position sensor 25 is configured to output signals to an actuator 40 based on the position of the manipulandum 20. An object 50 is removably or fixedly coupled to the manipulandum 20. The actuator 40 is coupled to a retainer 60. The retainer 60 houses an interface member 65 including a material that is configured to receive the object 50. The actuator 40 is configured to engage the retainer 60 in such a manner as to modify the density of the material of interface member 65 based on the position of the manipulandum 20 and/or the object 50, as will be described below.

In some embodiments of the invention, the medical procedure simulation device 10 includes a processor 30 that is configured to receive signals from the position sensor 25, and output signals to the actuator 40 and to a display 35 that is configured to output images associated with the medical procedure simulation as described below.

The display 35 is coupled to the processor 30 and is configured to output a simulated image based on data values associated with a position of the manipulandum 20 relative to, for example, the interface member 65. The processor 30 can be, for example, a commercially available personal computer, or a less complex computing or processing device that is dedicated to performing one or more specific tasks. For example, the processor 30 can be a terminal dedicated to providing an interactive virtual reality environment.

The processor 30, according to one or more embodiments of the invention, can be a commercially available microprocessor. Alternatively, the processor 30 can be an application-specific integrated circuit (ASIC) or a combination of ASICs, which are designed to achieve one or more specific functions, or enable one or more specific devices or applications. In yet another embodiment, the processor 30 can be an analog or digital circuit, or a combination of multiple circuits.

The processor 30 includes a memory component (not shown in FIG. 1). The memory component can include one or more types of memory. For example, the memory component can include a read only memory (ROM) component and a random access memory (RAM) component. The memory component can also include other types of memory that are suitable for storing data in a form retrievable by the processor 30. For example, electronically programmable read only memory (EPROM), erasable electronically programmable read only memory (EEPROM), flash memory, as well as other suitable forms of memory can be included within the memory component. The processor 30 can also include a variety of other components, such as for example, co-processors, graphics processors, etc., depending upon the desired functionality of the medical procedure simulation device 10.

The processor 30 is in communication with the memory component, and can store data in the memory component or retrieve data previously stored in the memory component.

The components of the processor 30 can communicate with devices external to the processor 30 by way of an input/output (I/O) component (not shown in FIG. 1). According to one or more embodiments of the invention, the I/O component can include a variety of suitable communication interfaces. For example, the I/O component can include, for example, wired connections, such as standard serial ports, parallel ports, universal serial bus (USB) ports, S-video ports, local area network (LAN) ports, small computer system interface (SCSI) ports, and so forth. Additionally, the I/O component can include, for example, wireless connections, such as infrared ports, optical ports, Bluetooth® wireless ports, wireless LAN ports, or the like.

The processor 30 is configured to receive signals from the position sensor 25 and output signals to the actuator 40. The processor 30 receives data values associated with the position (i.e., location and orientation) of the manipulandum 20 and, hence, the position and orientation of object 50 with respect to the interface member 65. The position signals can be absolute position signals or can be measured as a relative distance and direction from a predetermined reference point (e.g., the interface member 65, the retainer 60, or a support surface on which the device 10 is positioned). In alternative embodiments, a sensor or multiple sensors (not shown) can be disposed in the object 50, the interface member 65 or the retainer 60, and can be configured to determine the location of the manipulandum 20. Alternatively, the object 50, the interface member 65, or the retainer 60 can include a wireless or wired transmitter (not shown) that sends a position signal to the processor 30 to determine position information of the object 50 relative to the interface member 65. In some embodiments of the invention, the sensors can detect multiple degrees of freedom of the manipulandum (e.g., translation, pitch, yaw, rotation, etc.)

As the manipulandum 20 is moved from one position to another, the images output on the display 35 are updated based on the position signal. It is desirable for the position of the object 50 relative to the interface member 65 to be coordinated in a realistic sense with respect to the images output on the display 35. For example, when the material of the interface member 65 is a simulated pedicle of a vertebrae and the object 50 is a screw or a simulated screw, the images output on the display 35 should correspond accordingly. Images viewed on the display are obtained from actual spinal stabilization procedures and are reproduced based on position signals received from the position sensor 25. For example, in a spinal stabilization simulation, where the screws have been properly inserted, the image displayed can show a properly simulated screw.

The medical procedure simulation device 10 is configured to output haptic feedback based on the position of the manipulandum 20. The haptic feedback is designed to replicate the sensation that would be experienced by a user, for example, during a spinal stabilization procedure as described above. More specifically, as the user screws the object 50 into the material of the interface member 65, haptic feedback is output based on the position and orientation of the object 50. The position and orientation of the object 50 is related to the position and orientation of the manipulandum 20 by virtue of its coupling to the manipulandum 20. The manipulandum 20 can be rotated about an axis defined along the length of the manipulandum 20 and translate along that same axis while rotating. Depending upon the type of manipulandum 20 that is used, the manipulandum 20 can translate along the axis while a part or all of the manipulandum 20 does not rotate.

Referring to FIG. 2, a block diagram of a medical procedure simulation device according to an embodiment of the

invention is illustrated. The medical procedure simulation device **100** includes a housing **110** covered with a simulated skin **190**. The housing **110** can be, for example, a mannequin formed as a human body. The simulated skin **190** is configured to provide the sensation of skin penetration when inserting various elements of the device **100** as described below. The simulated skin **190** is a self-healing material in that the simulated skin is penetrable, but is able to return substantially to its original form once the inserted elements of the device **100** are removed.

The housing **110** defines an opening that is configured to receive at least one interface member **165** that includes a material configured to simulate a bone structure, such as a vertebrae. The material of the interface member **165** is configured to receive an actual or simulated pedicle screw **150**. The material is maintained in an interior portion of a retainer **160**. In embodiments of the medical procedure simulation device **100**, the interface member **165** material is fabricated from, for example, compressed sawdust such as that available from Sawbones® Worldwide in Vashon, Wash. Alternatively, the material can be fabricated from Selective Laser Sintering (SLS). SLS is a process by which three-dimensional parts are created by the fusing or sintering of powdered thermoplastic materials with the heat from an infrared laser beam. In this manner, various materials, such as compressed nylon, can be used. The material can be discarded after a single use, or may be used numerous times depending upon the durability of the material.

A screwdriver **120** is used to drive the screw **150** to penetrate the material of the interface member **165**. While being manipulated, the screws **150** are firmly attached to screwdriver **120**. The screwdriver **120** and the screw **150** are guided into the housing **110** through a shaft **180**. The shaft **180** can be fixed in the housing **110** or can be removably coupled such that the user of the device is able to simulate proper insertion of the shaft **180** as part of the simulated procedure.

A sensor **125** is configured to output a position signal based on the position of the screwdriver **120**. Because of the connection between the screwdriver **120** and the screw **150**, the location and orientation of the screw **150** can be determined based on the position signal associated with the position of the screwdriver **120** and/or the position and orientation of the shaft **180**. The sensor **125** can incorporate any known methods appropriate for tracking the position of the screwdriver **120**. For example, the sensor may be a visual sensor configured to track marks on the screwdriver **120** or an extension (not shown) coupled to the screwdriver **120**. Alternatively, a mechanical arm (not shown) can be coupled at one end to the screwdriver **120** and at another end to the position sensor **125**. A mechanical arm such as the one used in the Microscribe® device available from Immersion Corporation in San Jose, Calif. is suitable for some embodiments of the invention. An example of such a mechanical arm is disclosed in U.S. patent application Ser. No. 09/687,923, now U.S. Pat. No. 6,697,748, which is incorporated herein by reference.

The position sensor **125** is coupled to an actuator **140** and is configured to output position signals. Actuation signals based on the position signals are then sent to the actuator **140**. Alternatively, if the actuator **140** has an embedded processor, the position signals are sent directly to the actuator **140**. The actuator **140** is coupled to the retainer(s) **160** and is configured to output haptic feedback based on the position signal by applying a compressive force to the material of the interface member **165**.

The medical simulation device **100** can be used, for example, to train users to orient the screws **150** to align properly with the pedicles of a vertebrae. In an actual procedure,

as the screw is successfully embedded in the vertebrae, the screw encounters varying density bone that is visible on a fluoroscope display and is perceptible to the user's sense of touch. The medical procedure simulation device **100** simulates the sensation of encountering varying bone density by varying the density of the material of the interface member **165**.

Referring to FIG. 3, an example of an interface member **165** is illustrated in which the material includes multiple layers **171**, **172**, **173** and **174**. The density of the material in layers **171**, **172**, **173** and **174** may be the same or different. As illustrated in FIGS. 2 and 3, the screw **150** is configured to penetrate the layers **171**, **172**, **173** and **174** of interface member **165**. To further vary the density of the material of the interface member **165**, the actuator **140** includes a clamp or band **144** that encircles the interface member **165**. As discussed above, the actuator **140** is configured to vary the density of the material based on the position signal received from the position sensor **125**. Although the clamp or band **144** is shown in FIG. 3 as surrounding layer **172** only, in other embodiments the clamp or band **144** can surround more or all layers of the material of the interface member **165**.

In use, as the screw **150** is manipulated and penetrates the material of the interface member **165**, the diameter of the clamp **144**, and likewise the opening defined by the clamp **144**, can vary. The diameter of the clamp **144** may be varied by actuation of a motor (not shown) coupled to the clamp **144**. With the varying diameter of the clamp **144**, the compressive force applied to the material of the interface member **165** varies as well. Accordingly, haptic feedback is provided, thereby providing the sensation of a variable density bone structure.

The density of the material of interface member **165** can be varied to simulate various conditions. For example, if the screw **150** is not properly inserted (e.g., inserted at an improper angle) the clamp **140** will quickly loosen to simulate shearing of the bone structure. Alternatively, if the screw **150** is properly inserted, the clamp **140** will compress the material to simulate dense bone structure until the screw **150** moves an appropriate distance, at which point the clamp will release to simulate entry of the screw **150** into the less dense portion of the bone structure.

An alternative embodiment of an interface member for use with the medical simulation device **100** is illustrated in FIG. 6. The interface member **665** includes a structural member **667** that simulates various elements of the spine that could be encountered when performing various medical procedures. The material of the interface member **665** can be fabricated from varying density material. For example, a first portion **667** of the material can be fabricated using a material having a density and a second portion **669** of the material can have a density different from the density of the first portion **667**. In the illustrated embodiment, the actuator **644** includes a band that is coupled to the retainer **660**. Alternatively, the band is integrally formed as part of the retainer **660**. The density of the first portion **667** of the material and the second portion **669** of the material can be further varied by actuation of the band based on the position signal received by the actuator **644** as described above.

An alternative embodiment of an interface member for use with the medical simulation device **100** is illustrated in FIGS. 4 and 5. FIG. 4 illustrates interface member **465** in a decompressed condition and FIG. 5 illustrates interface member **465** in a compressed condition. In the illustrated embodiment, the interface member **465** defines a chamber **468** including compressible beads **469** that can be compressed and decompressed to simulate various conditions based on the position

of the screwdriver **120**. The beads **469** can be fabricated from, for example, polystyrene, nylon (polyamide) powder, sugar, etc. FIGS. **4** and **5** are for illustrative purposes only and a greater bead density than that shown would be required to pressurize the interface member **465** to a degree sufficient to simulate bone density.

As illustrated, the density of the beads in the interface member **465** can be modified via vacuum pump **440**. When the area inside the chamber **468** is evacuated, the external air pressure causes the beads to compress. The chamber **468** contains a sufficient amount of compressible beads to pressurize the interface member **465**. As discussed above, as the screw **150** penetrates the interface member, the density can be varied to output haptic feedback based on the position of the screwdriver **120**. The chamber **468** has a seal sufficient to prevent air from leaking into or escaping from the chamber **468** at the entry point of the screw **150**.

The density of the beads **469** can be varied by modifying the size of the chamber **468**. In such an embodiment, this chamber **468** is defined by a flexible housing that collapses around the beads **469** to increase the density. Likewise, the flexible housing can be expanded to decrease the density.

CONCLUSION

While various embodiments of the invention have been described above, it should be understood that they have been presented by way of example only, and not limitation. Thus, the breadth and scope of the invention should not be limited by any of the above-described embodiments, but should be defined only in accordance with the following claims and their equivalence.

The previous description of the embodiments is provided to enable any person skilled in the art to make or use the invention. While the invention has been particularly shown and described with reference to embodiments thereof, it will be understood by those skilled in art that various changes in form and details may be made therein without departing from the spirit and scope of the invention.

For example, although the manipulandum **20** is described as being a screwdriver **120** in some embodiments of the invention, in an alternative embodiment the manipulandum can be any tool that is configured to move the object into the material of the interface member. For example, the manipulandum can be a drill, a hammer, a pneumatic hammer, a pneumatic or hydraulic press, a pneumatic or hydraulic drill or screwdriver, etc.

Although the processor **30** is described above as being directly coupled to the manipulandum **20** and the actuator **40**, in an alternative embodiment, the processor **30** can be coupled to the medical procedure simulation device **10** via a network.

Additionally, although the position sensor **125** is described above as being configured to output position signals based on the position of the screwdriver **120**, in some alternative embodiments, the position sensor is configured to track the position of the screws **150** directly. In a further alternative embodiment, sensors embedded in the interface member **165** can replace or augment the position sensor **125**.

Although the material of the interface member **165** is described above as being disposed in the retainer **160**, in some alternative embodiments, the retainer **160** need not be used. In other words, the actuator **140** can be directly coupled to the material and apply a compressive force directly to the material.

Although the medical procedure simulation device **110** is not illustrated as including the various rods and external

structures associated with the actual device illustrated in FIG. **7**, the simulation device can include any or all of the elements associated with the actual device whether illustrated or not.

Although the manipulandum **20** and object **50** are disclosed as being separate elements, the manipulandum **20** and object **50** can be fixedly coupled as discussed above and thus considered a single element. In this manner, the manipulandum can penetrate the interface member when the object is considered a part of the manipulandum.

Although the clamp **144** is illustrated as a thin band that surrounds only a portion of the interface member **165**, the clamp **144** may be wide enough to cover the entire length of the material of the interface member **165**. Moreover, while only one actuator is illustrated, the medical procedure simulation device **100** may include more than one actuator. Each actuator may be associated with a different interface member, or multiple actuators may be arranged to selectively compress a single interface member.

Although the housing **110** is disclosed above as having an opening to receive the interface members **165**, in some alternative embodiments, the interface members may be coupled directly to the simulated skin **190** and a housing **110** is not needed.

Although the interface member **465** is described as having beads **469** that are compressed by decreasing the volume of chamber **468**, in alternative embodiments, the beads **469** can be pre-compressed by means of a band placed around chamber **468**. For example, the beads **469** can be initially pressurized a predetermined amount and then either further pressurized by pressurizing the chamber as discussed above, or depressurized by expanding the chamber against the band placed around the chamber.

What is claimed is:

1. A device, comprising:

an interface member including a compressible material of selectively variable density;

a manipulandum movable in a degree of freedom, the manipulandum configured to cause an object to penetrate the material;

a sensor configured to output a position signal based on the depth of penetration of the object within the material; and

an actuator configured to:

apply a first compressive force to the material to change the density of the material within at least a portion of the interface member in response to the position signal, wherein the change in density of the material imparts a haptic effect to the manipulandum, and

apply a second compressive force to the material substantially simultaneously with the first compressive force, wherein the first compressive force is different from the second compressive force.

2. The device of claim **1**, wherein the material includes a plurality of compressible beads.

3. The device of claim **1**, wherein the material includes a plurality of polystyrene beads.

4. The device of claim **1**, wherein the interface member includes a simulated bone structure.

5. The device of claim **1**, wherein the manipulandum is rotatable about an axis defined along a length of the manipulandum when the manipulandum has penetrated the material.

6. The device of claim **1**, wherein the actuator is a clamp coupled to the interface member, the clamp configured to decrease a volume of the interface member to change the density of the material.

7. The device of claim **1**, wherein the actuator is a vacuum coupled to the interface member.

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8. The device of claim 1, the actuator being a first actuator, the device further comprising a plurality of actuators including the first actuator, each actuator from the plurality of actuators being an individually actuatable clamp.

9. The device of claim 1, wherein the material comprises a plurality of layers, and wherein:

the actuator is further configured to apply the first compressive force to a first layer of the plurality of layers, and apply the second compressive force to a second layer of the plurality of layers.

10. A device, comprising:

a retainer defining an interior in which a compressible material is disposed and having a selectively variable density when a compressible force is applied thereto;

a manipulandum movable in a degree of freedom, the manipulandum configured to cause an object to penetrate the material;

a sensor configured to output a position signal based on the depth of penetration of the object within the material; and

an actuator coupled to the retainer, the actuator configured to:

apply a first compressible force to the material to change the density of the material in response to the position signal, wherein the change in density of the material imparts a haptic effect to the manipulandum, and

apply a second compressible force to the material substantially simultaneously with the first compressible force, wherein the first compressible force is different from the second compressible force.

11. The device of claim 10, wherein the manipulandum includes a first portion and a second portion, the second portion configured to be removably coupled to the object.

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12. The device of claim 10, wherein the manipulandum is configured to move in a rotary degree of freedom about an axis, and move simultaneously along the axis.

13. The device of claim 10, wherein the interface member includes a simulated pedicle of a vertebrae.

14. The device of claim 10, wherein the interface member includes a simulated bone structure.

15. The device of claim 10, wherein the retainer is configured to compress the material in response to actuation of the actuator.

16. The device of claim 10, wherein the manipulandum is rotatable about an axis defined along a length of the manipulandum when the manipulandum has penetrated the material.

17. The device of claim 10, wherein the retainer is a clamp having an opening, the actuator including a motor configured to modify a size of the opening based on the position signal.

18. The device of claim 10, wherein the manipulandum is a screwdriver and the object is a screw.

19. The device of claim 10, further comprising:

a guide configured to receive at least a portion of the manipulandum, the guide being removably coupled adjacent to the retainer.

20. The device of claim 10, wherein the manipulandum is movable in two degrees of freedom.

21. The device of claim 10, wherein the compressible material is not rigid.

22. The device of claim 10, wherein the material comprises a plurality of layers, and wherein:

the actuator is further configured to apply the first compressive force to a first layer of the plurality of layers, and apply the second compressive force to a second layer of the plurality of layers.

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