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Rotstein

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(54) **OCCLUSION DETECTION FOR AN INFUSION PUMP SYSTEM**

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A61M 31/00 (2006.01)
A61M 1/00 (2006.01)

(52) **U.S. Cl.**
USPC **604/67**; 604/151

(58) **Field of Classification Search**
USPC 604/67, 151, 253, 93.01, 65, 500, 131, 604/181, 189, 110; 73/715
See application file for complete search history.

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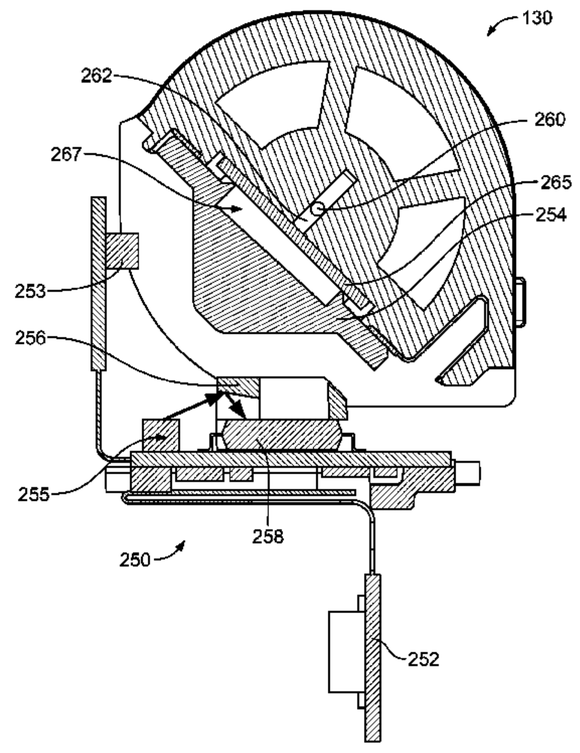
(57) **ABSTRACT**

Some embodiments of an infusion pump system include an occlusion detection system to detect when an occlusion exists in the fluid path between the medicine reservoir and the infusion site located, for example, on the user's skin. The occlusion detection system can be configured to self-calibrate in a manner that accounts for changes in environmental conditions, such as ambient temperature, pressure, or the like, so that the occlusion detection system provides reliable feedback to a user as to the occluded or non-occluded state of the medicine flow path.

20 Claims, 14 Drawing Sheets



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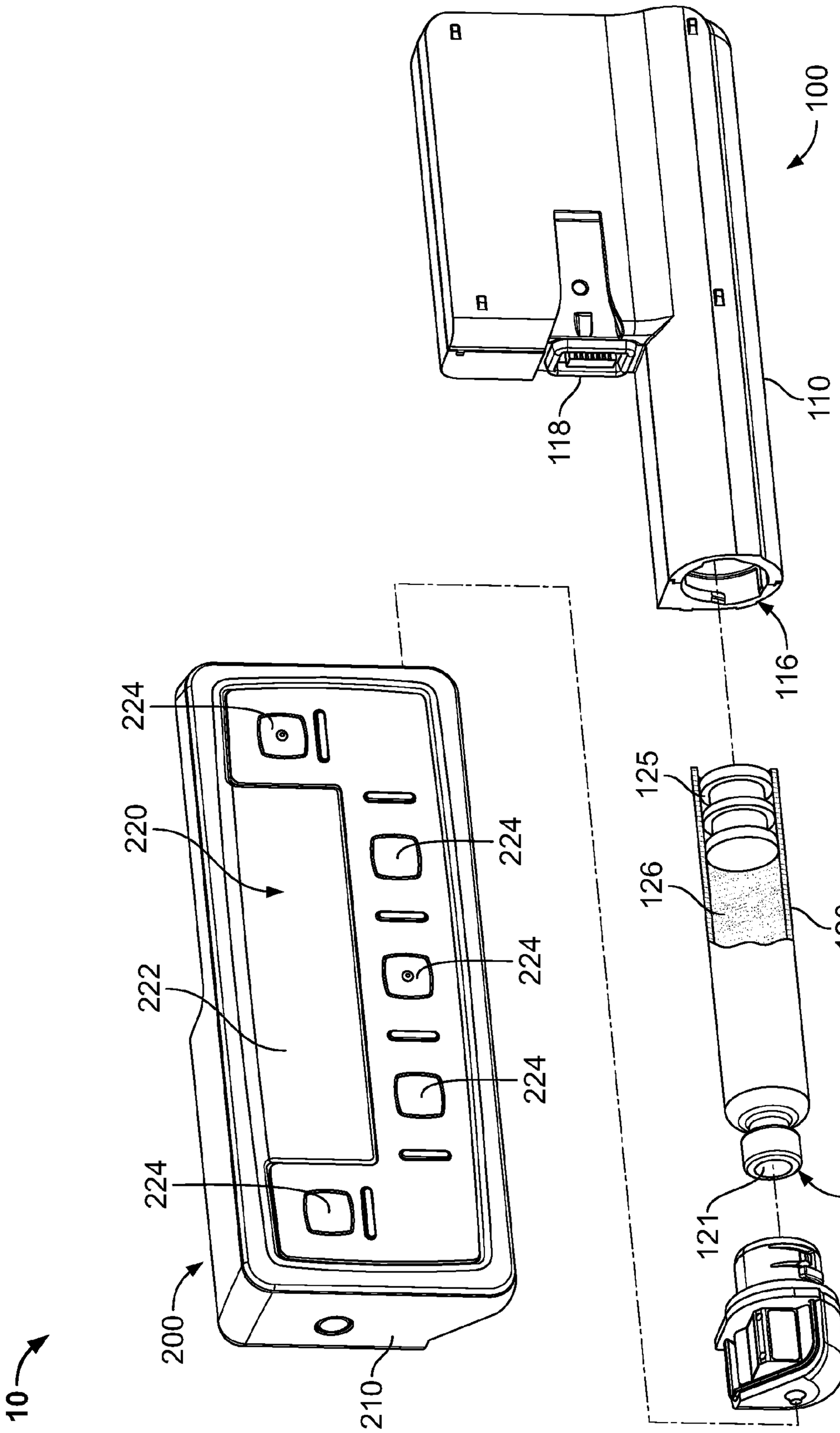
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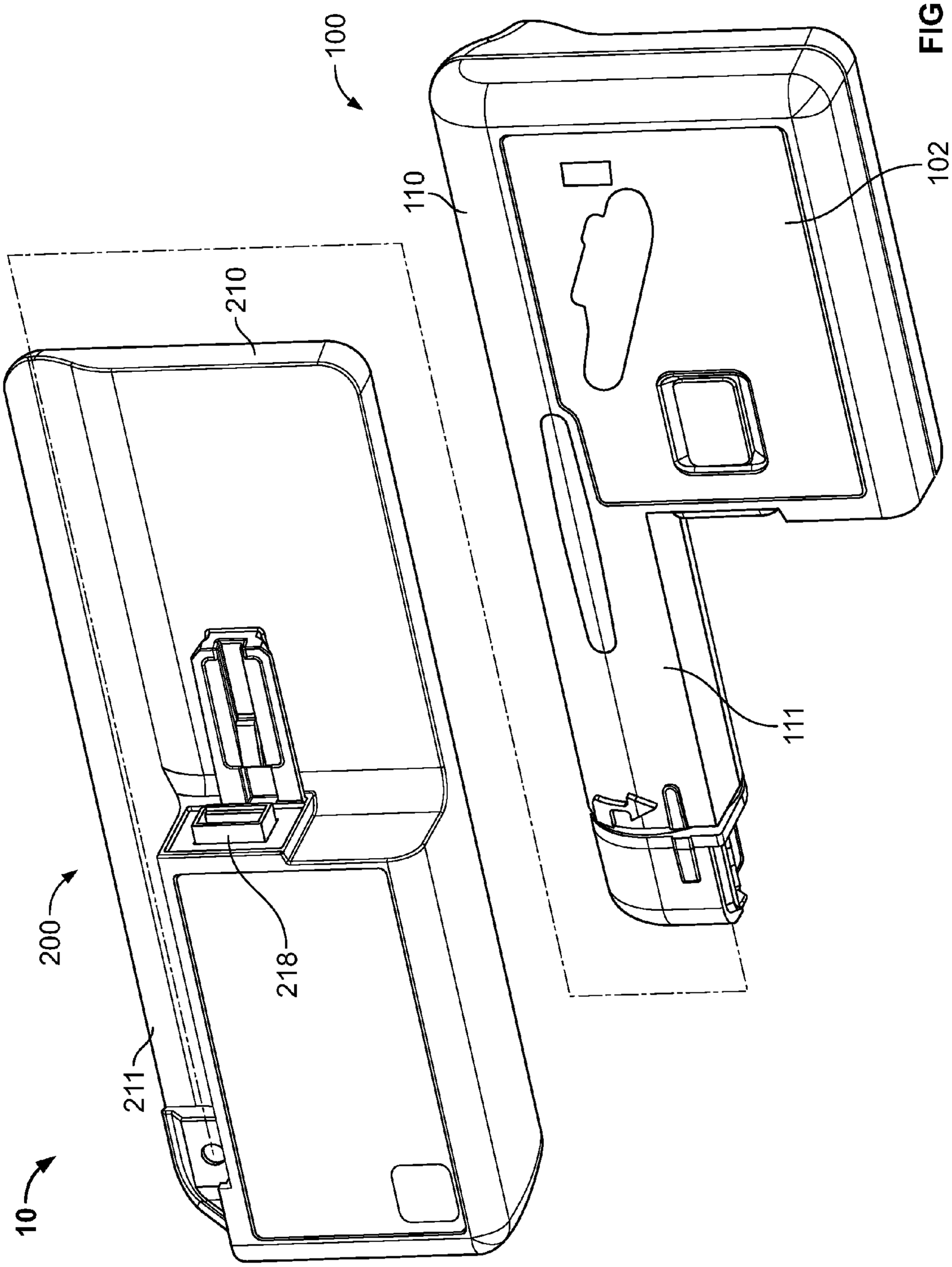
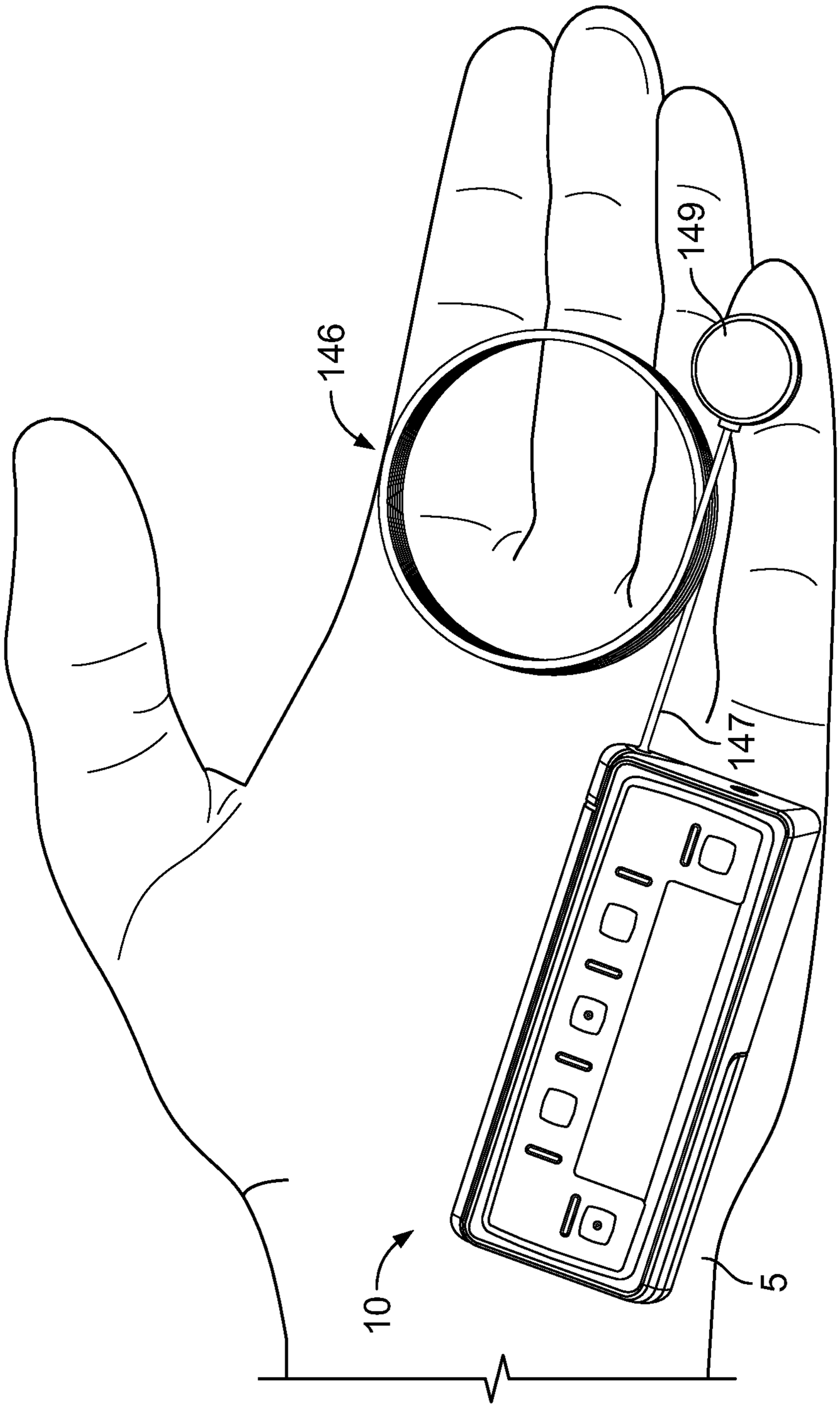
FIG. 1

FIG. 2





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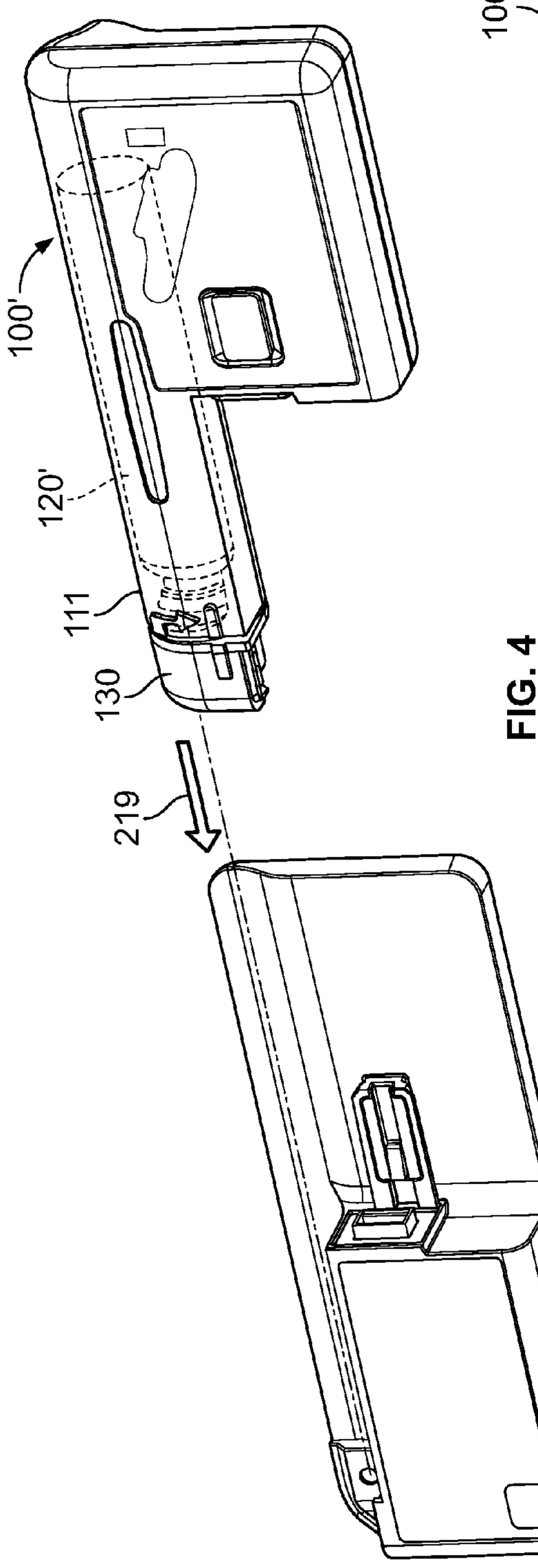

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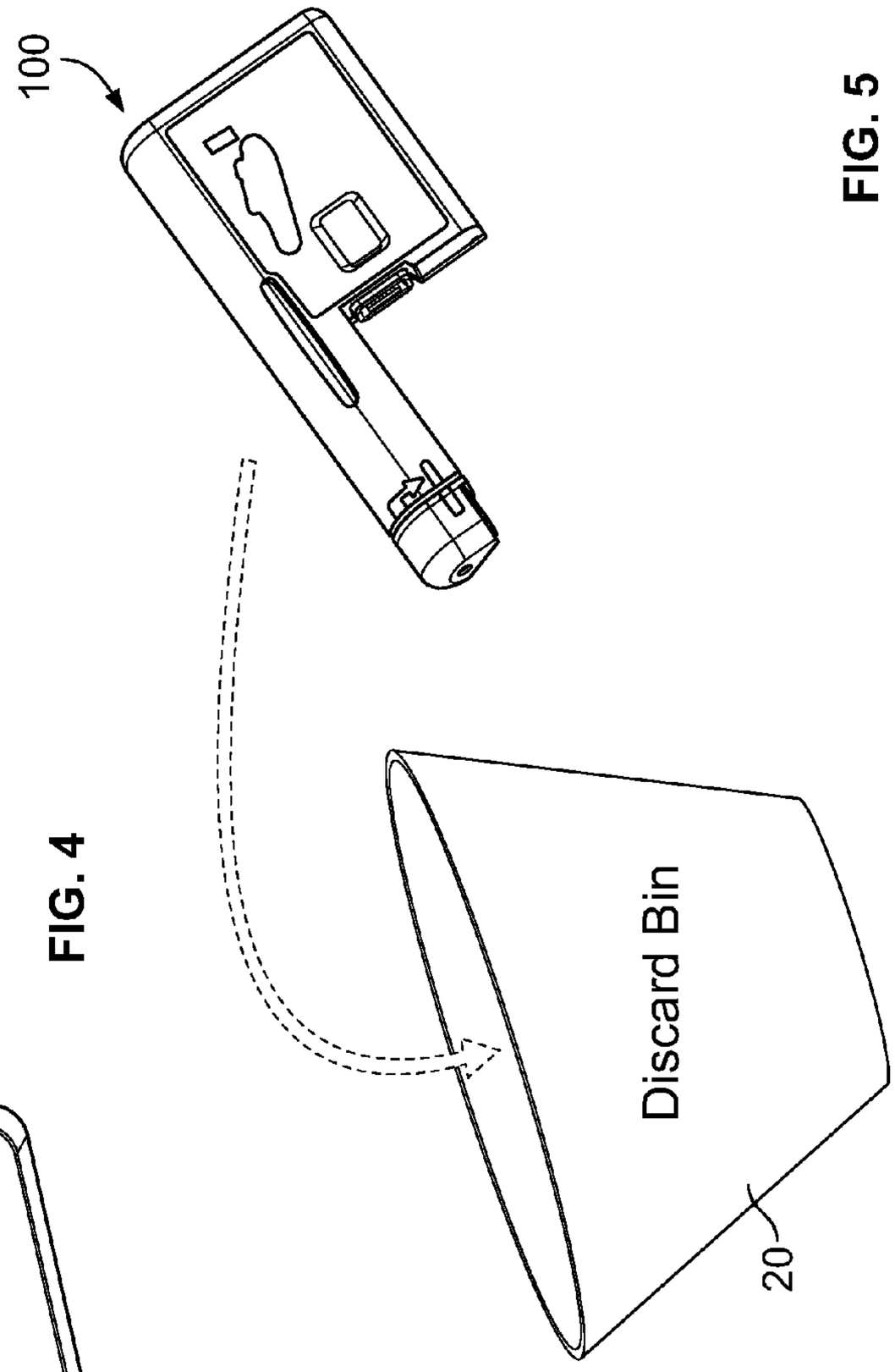

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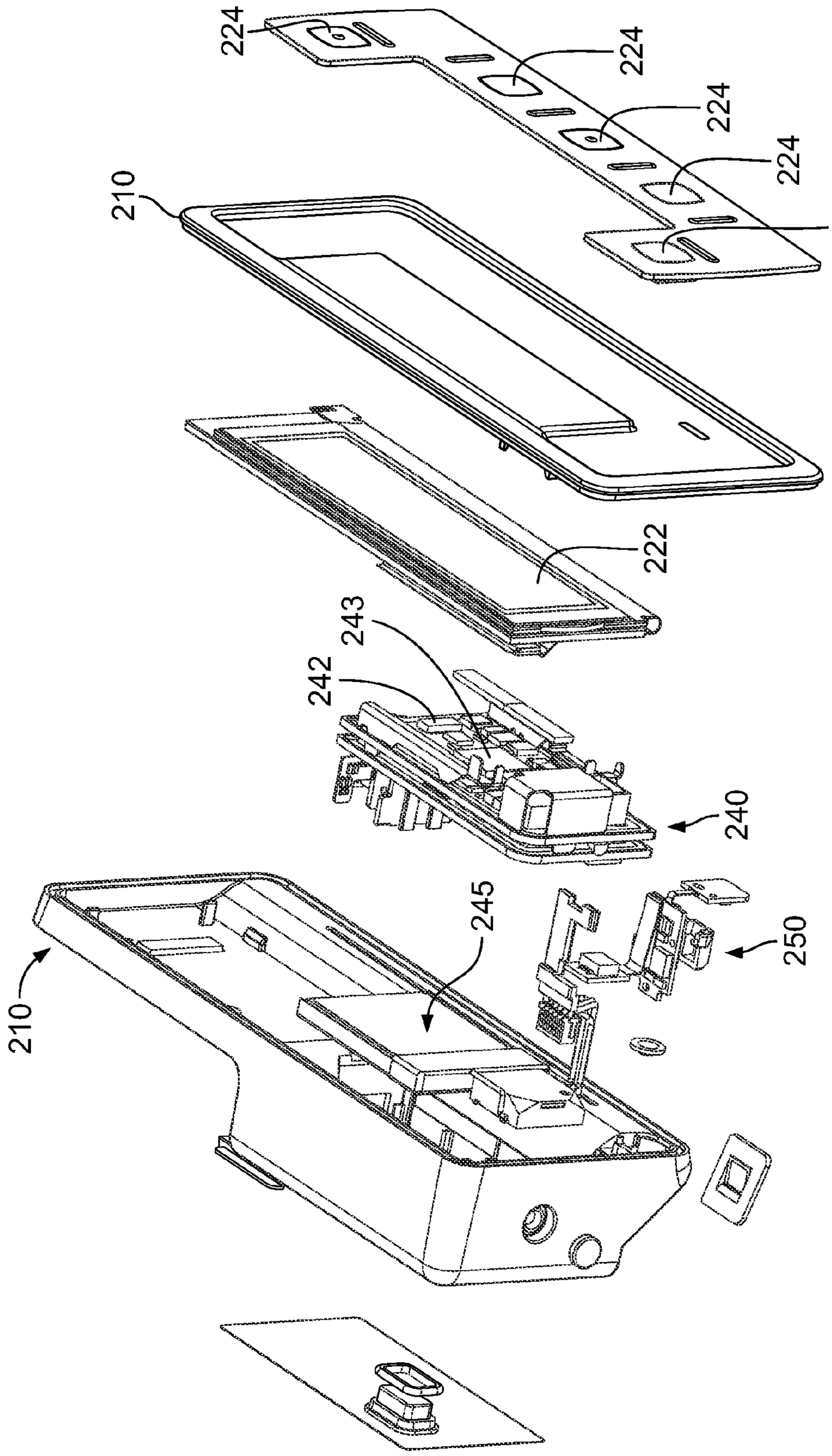
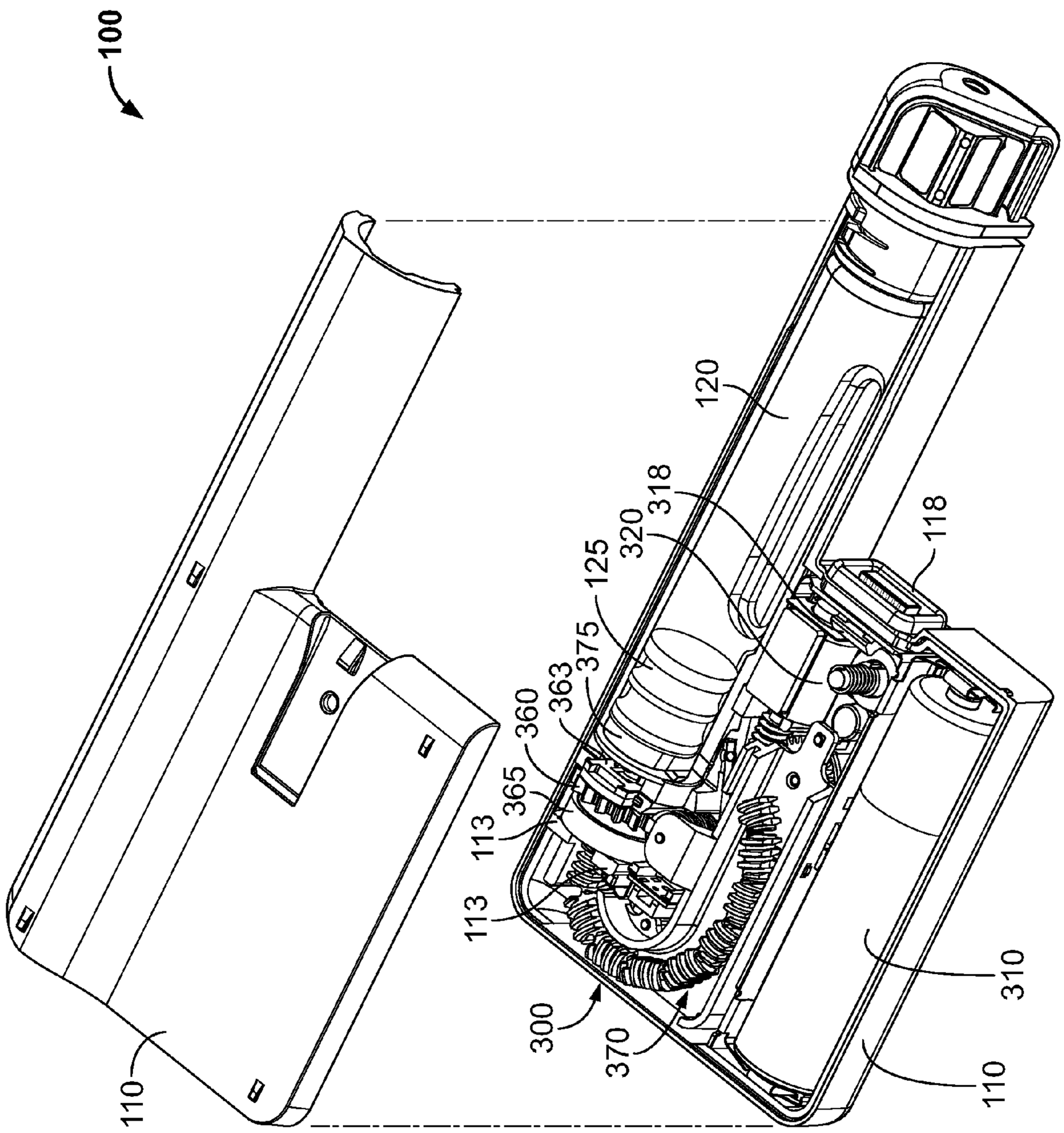
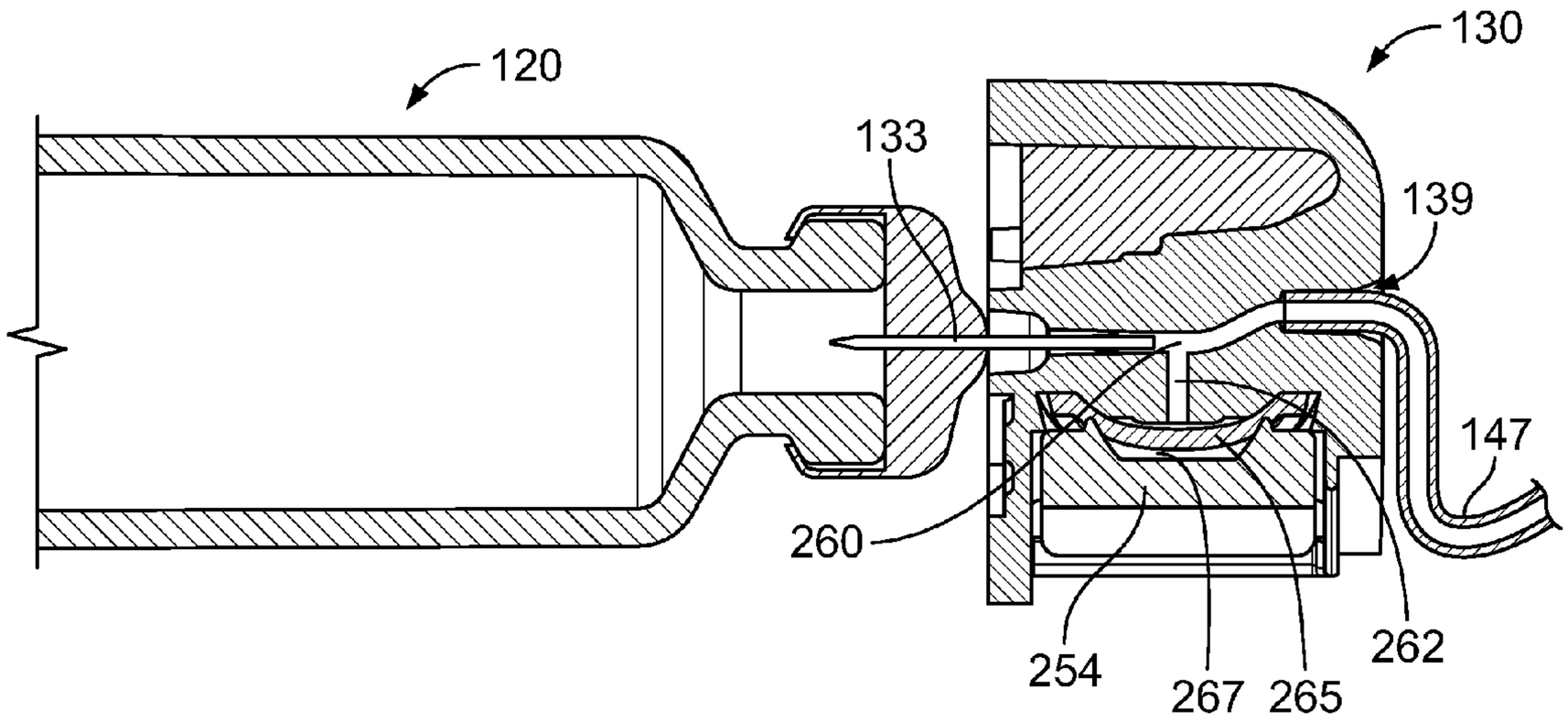


FIG. 6

FIG. 7

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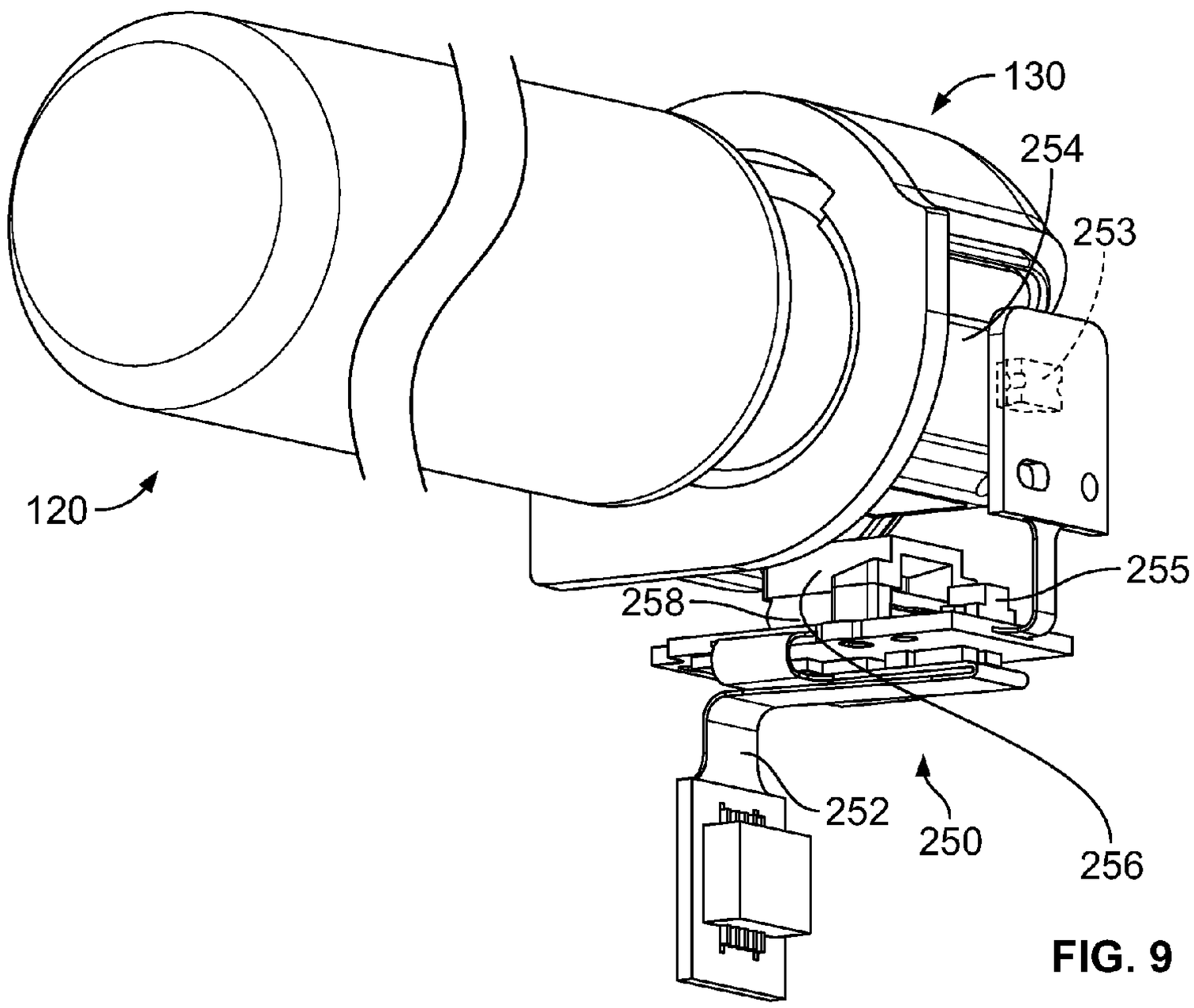
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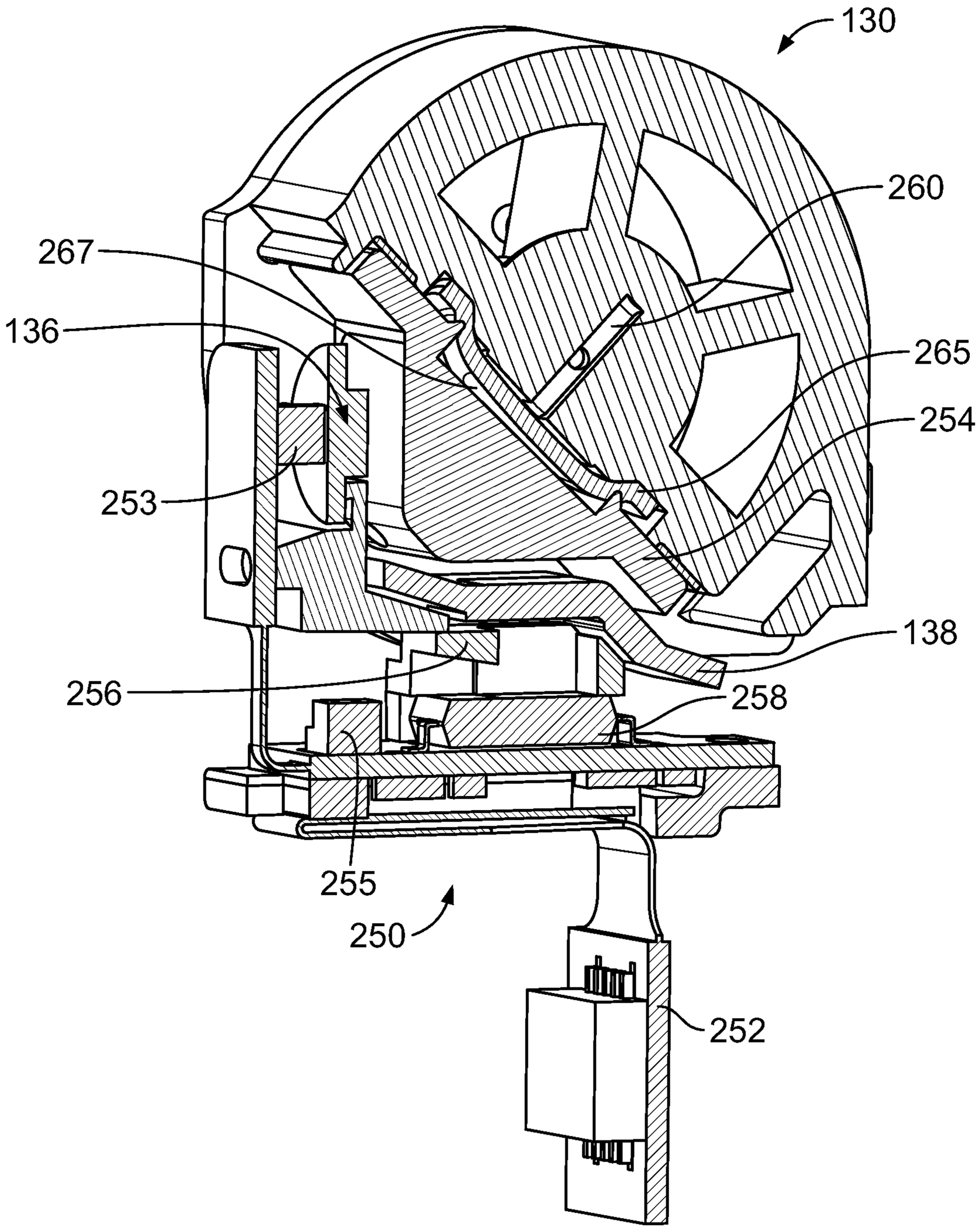


FIG. 10

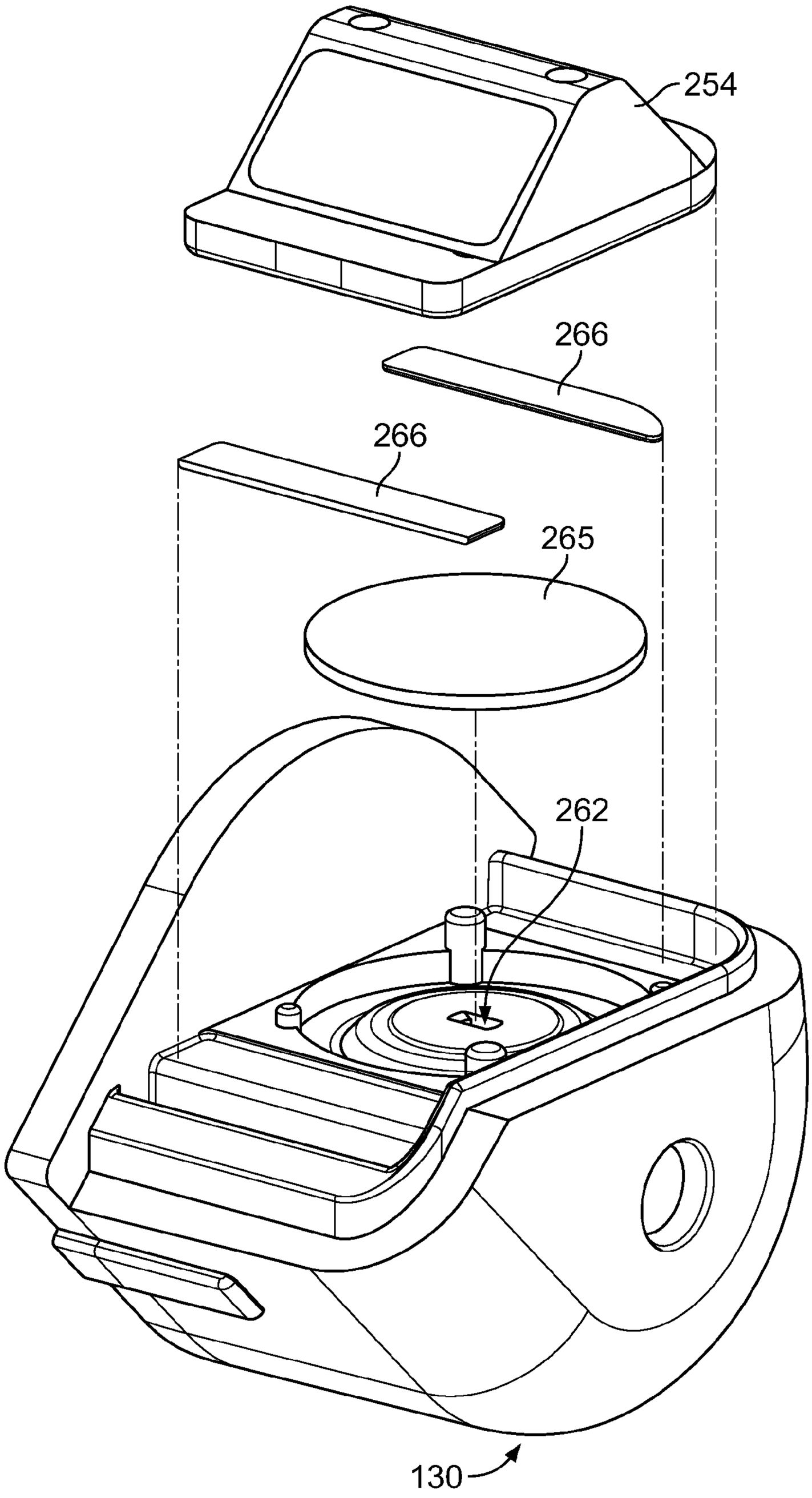


FIG. 11

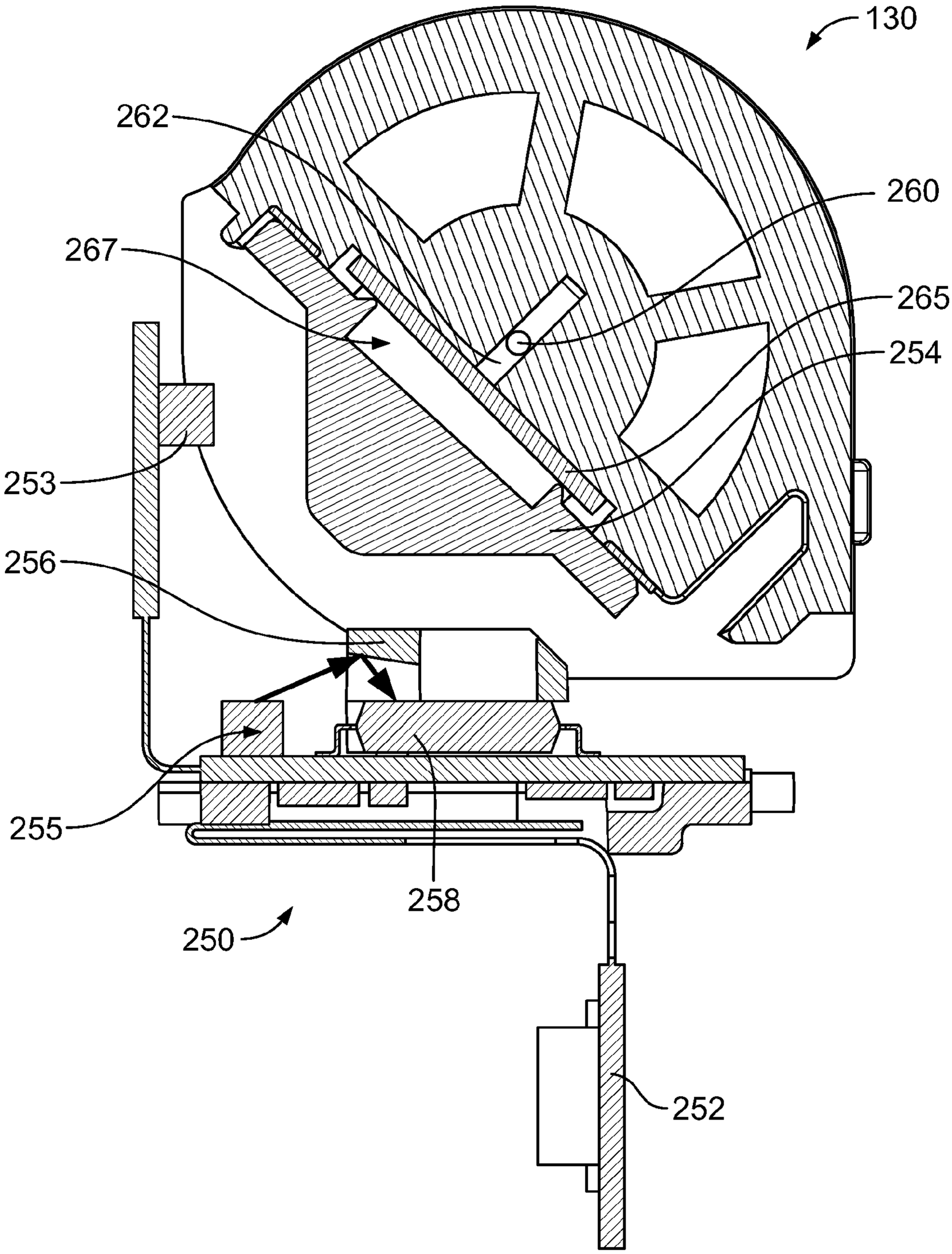


FIG. 12

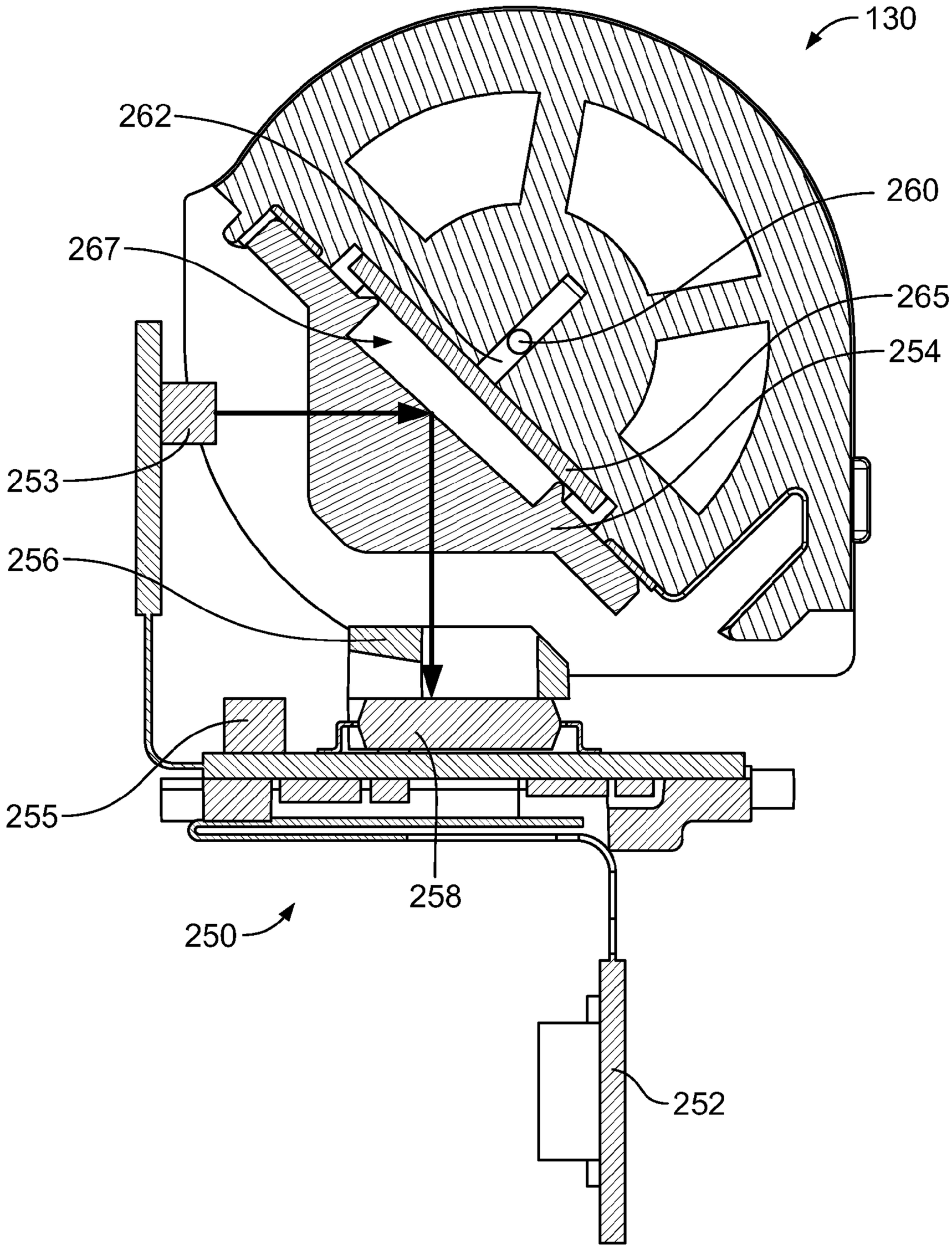


FIG. 13

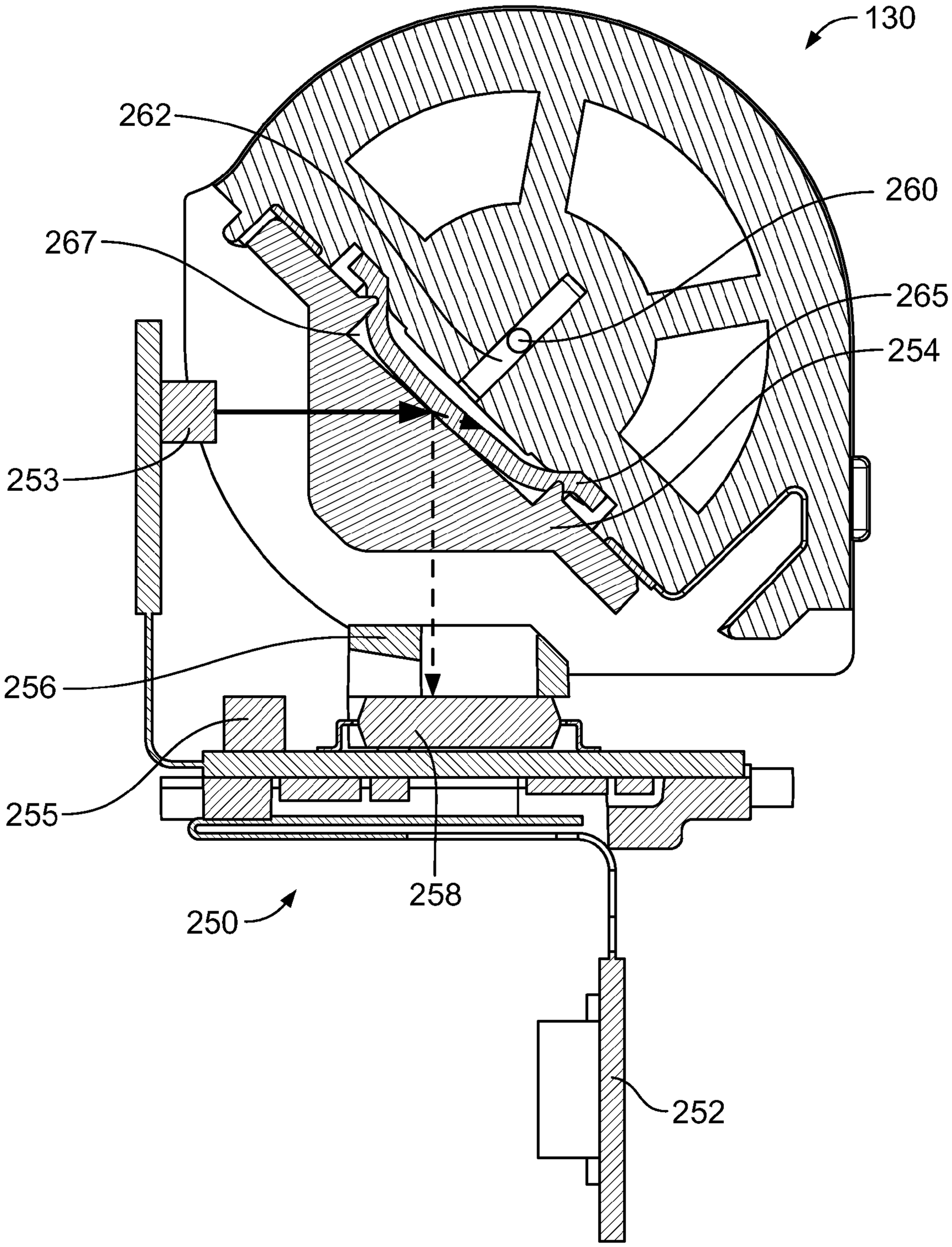
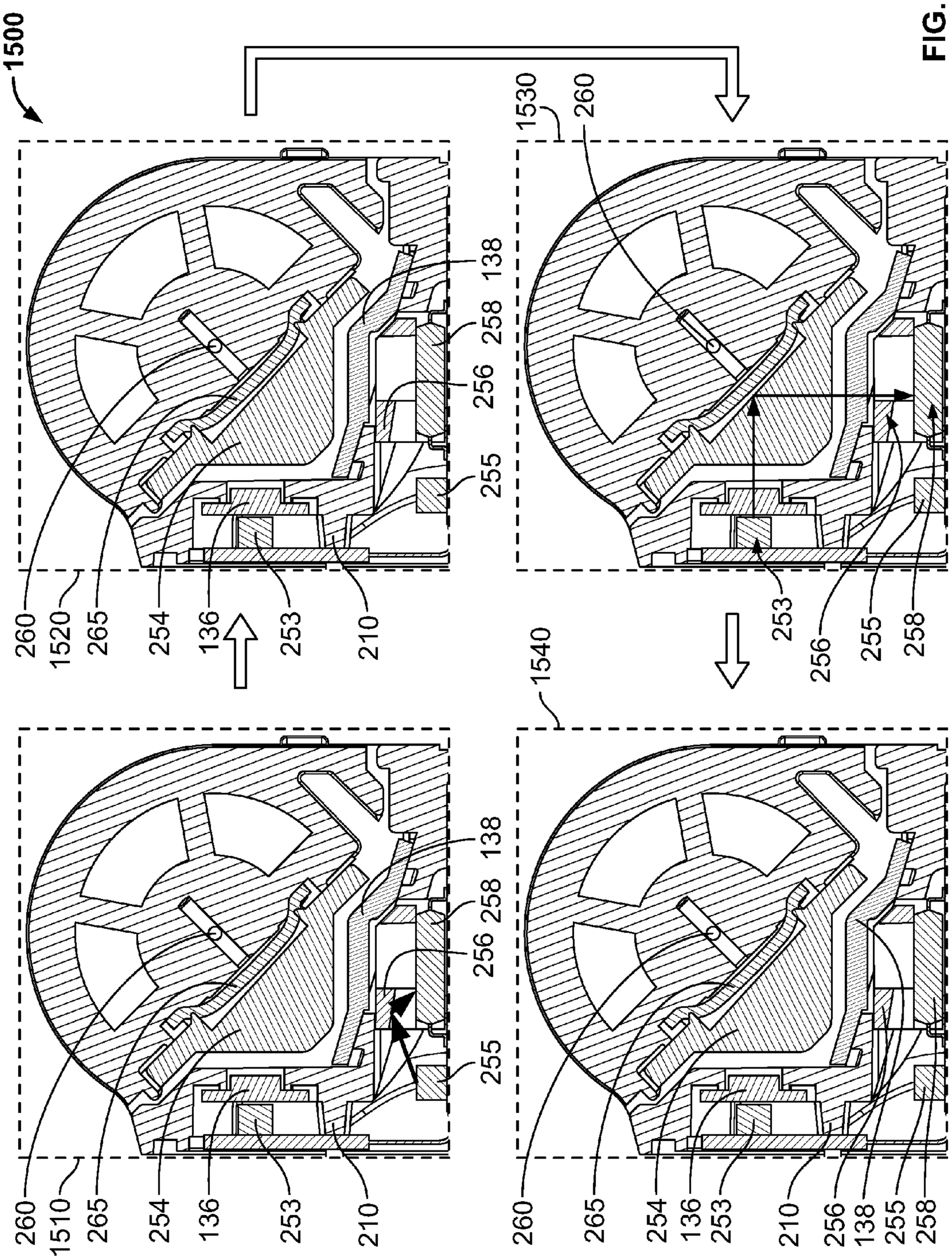


FIG. 14

FIG. 15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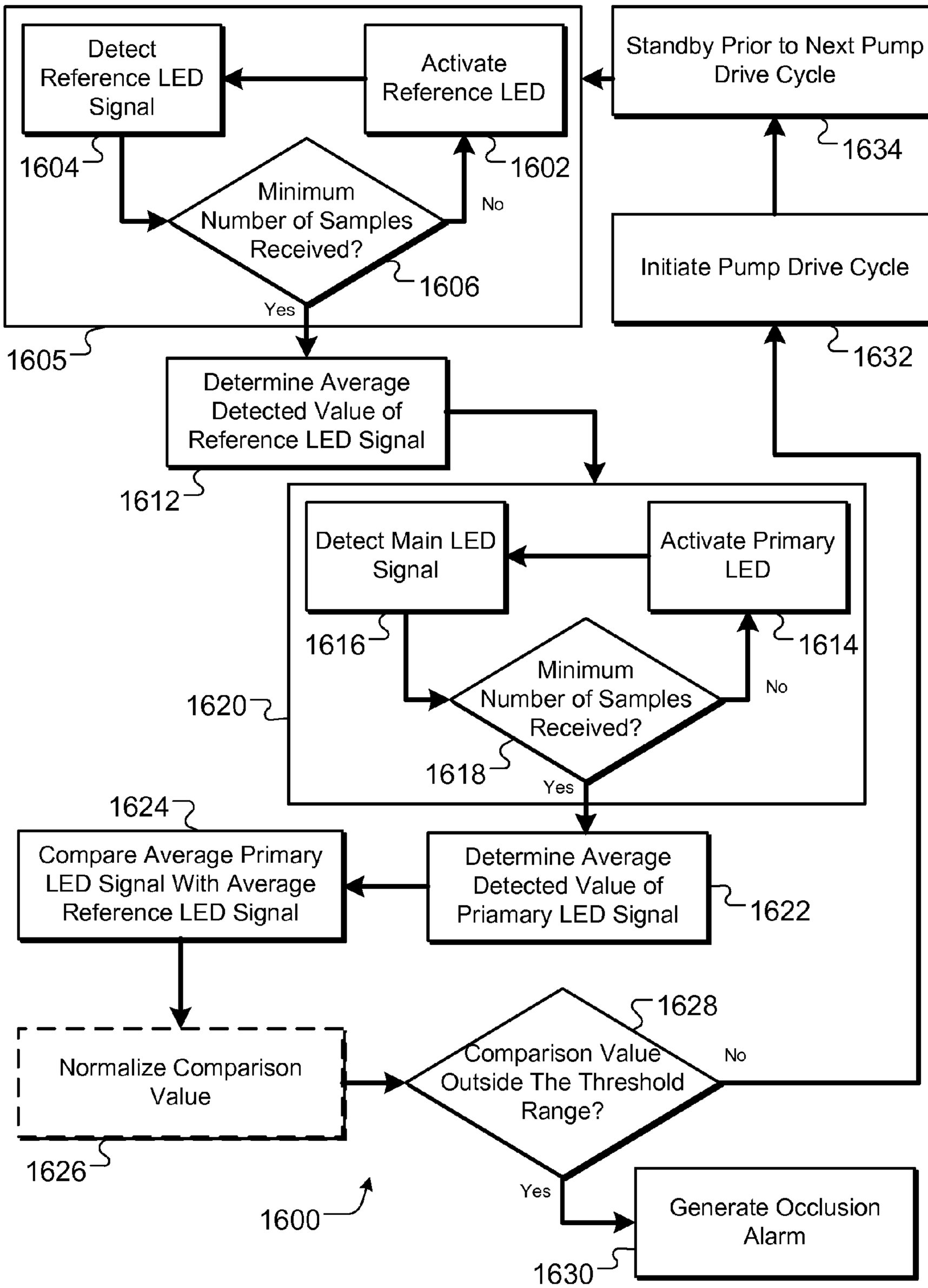
Detect Reference LED Signal
Activate Reference LED
Standby Prior to Next Pump Drive Cycle
1604
1602
1634
Minimum Number of Samples Received?
No
1606
Yes
1605
Initiate Pump Drive Cycle
1632
Determine Average Detected Value of Reference LED Signal
1612
Detect Main LED Signal
Activate Primary LED
1616
1614
1620
Minimum Number of Samples Received?
No
1618
Yes
1624
Compare Average Primary LED Signal With Average Reference LED Signal
Determine Average Detected Value of Priamary LED Signal
1622
Normalize Comparison Value
1628
Comparison Value Outside The Threshold Range?
No
1626
Yes
1600
Generate Occlusion Alarm
1630

FIG. 16

OCCLUSION DETECTION FOR AN INFUSION PUMP SYSTEM

TECHNICAL FIELD

This document relates to an infusion pump system, such as a portable infusion pump system for dispensing insulin or another medication.

BACKGROUND

Pump devices are commonly used to deliver one or more fluids to a targeted individual. For example, a medical infusion pump device may be used to deliver a medicine to a patient as part of a medical treatment. The medicine that is delivered by the infusion pump device can depend on the condition of the patient and the desired treatment plan. For example, infusion pump devices have been used to deliver insulin to the vasculature of diabetes patients so as to regulate blood-glucose levels.

Some traditional infusion pump devices may include an occlusion detection system for purposes of determining when the medicine dispensation is inadvertently interrupted or interfered. If the medicine dispensation path to the user is occluded, the user may receive no dosage or a lower dosage of the medicine. Some occlusion detections systems for infusion pumps can be configured as a "dry side" detector in which a sensor is positioned along a component of the drive system to detect a malfunction or change in pressure. Other occlusion detection systems for infusion pumps can be configured as a "wet side" detector in which characteristics of the fluid flow path are monitored. In some circumstances, the occlusion detection systems may be sensitive to environmental conditions (e.g., ambient temperature, pressure, or the like) in a manner that could cause false indications of a flow path occlusion.

SUMMARY

Some embodiments of an infusion pump system include an occlusion detection system to detect when an occlusion exists in the fluid path between the medicine reservoir and the infusion site located, for example, on the user's skin. Such an occlusion may occur, for example, when the fluid flow line (e.g., a cannula, infusion set tubing, or the like) is kinked. The occlusion detection system can be configured to account for changes in environmental conditions, such as ambient temperature, pressure, or the like, so that the occlusion detection system provides reliable feedback to a user as to the occluded or non-occluded state of the medicine flow path. As such, the occlusion sensor can be used to indicate when the fluid is flowing or not flowing, thereby permitting the infusion pump system to communicate an alarm to the user if an occlusion exists.

Particular embodiments described herein include an occlusion sensor system for detecting an occlusion in a flow path from an insulin infusion pump system. The occlusion sensor system may include a fluid channel that at least partially defines an insulin flow path between an insulin reservoir and an output port. The system may also include a flexible membrane in fluid communication with the fluid channel so that fluid pressure in the fluid channel acts upon the flexible membrane. The system may further include an air cavity positioned adjacent to the flexible membrane and generally opposite the fluid channel. The system may include a light transmissive member adjacent to the air cavity. The light transmissive member may be arranged opposite the flexible membrane such that fluid pressure in the fluid channel above a threshold value causes the flexible membrane to deform into the air cavity and toward the light transmissive member. The system may also include a primary light emitter configured to align with the light transmissive member and emit light into the light transmissive member. The system may further include a light sensor configured to align with the light transmissive member and receive light from the primary light emitter that passes through the light transmissive member. The system may include a reference light emitter configured to emit light that is received by the light sensor, wherein the reference light emitter is spaced apart from the primary light emitter.

Some embodiment described herein may include occlusion sensor system for an infusion pump system including a reusable controller device that is removably attachable to a disposable single-use pump device that defines a space to receive medicine therein. The occlusion sensor system may include a primary light emitter, a reference light emitter, and a light sensor arranged in the reusable controller device. The primary light emitter, the reference light emitter, and the light sensor may be in electrical communication with control circuitry housed inside the reusable controller device. The system may also include a light transmissive member arranged in the disposable single-use pump device. The light transmissive member may be aligned with the primary light emitter and the light sensor when the reusable controller device is removably attached to a disposable single-use pump device. The light sensor may be positioned relative to the light transmissive member so as to receive light from the primary light emitter that passes through the light transmissive member in response to activation of the primary light emitter. Also, in response to activation of the reference light emitter, the light sensor may receive light emitted from the reference light emitter without passing through the light transmissive member.

Particular embodiments described herein may include an occlusion sensor system for detecting an occlusion in a flow path from an insulin infusion pump system. The occlusion sensor system may include a primary light emitter configured to emit light toward an insulin flow path. The system may also include a light sensor configured to receive at least a portion of the light from the primary light emitter after the light is emitted toward the insulin flow path. The light sensor may output an electrical signal in response to receiving light. The system may further include a reference light emitter configured to emit light that is received by the light sensor. The reference light emitter may be separate from the primary light emitter. The system may further include control circuitry electrically connected to the primary light emitter, the reference light emitter, and the light sensor. The control circuitry may compare a first value indicative of light detected at the light sensor from the primary light emitter to a second value indicative of light detected at the light sensor from the reference light emitter. In response to the comparison of the first value to the second value being outside of a threshold range, the control circuitry may generate an occlusion alarm for output via a user interface.

Some embodiments include a method for detecting an occlusion in a flow path from an infusion pump system. The method may include activating a reference light emitter to direct light toward a light sensor housed in an infusion pump system. The light sensor may generate an electrical signal in response to receiving light from the reference light emitter. The method may also include determining a first value indicative of light detected at the light sensor from the reference light emitter. The method may further include activating a primary light emitter to direct toward a medicine flow path for

the infusion pump system. The light sensor may receive a least a portion of the light emitted from the primary light emitter. The method may include determining a second value indicative of light detected at the light sensor from the primary light emitter. The method may also include determining if an occlusion exists in the medicine flow path based at least in part on a comparison of the second value to the first value.

Some or all of the embodiments described herein may provide one or more of the following advantages. First, the infusion pump system may include an occlusion detection system configured to reliably detects occlusions in the medicine flow path even when the infusion pump system is exposed to significant changes in environments conditions. For example, the occlusion detection system can be configured to self-calibrate and thereby account for changes in ambient temperature so that the occlusion detection system provides reliable feedback even when the infusion pump system is carried in low-temperature conditions. As such, the occlusion detection system can provide notice to the user if he or she is receiving no dosage or a lower dosage of the medicine due to an occlusion in the medicine flow path.

Second, particular embodiments of the occlusion detection system may employ at least two different light emitters for each light sensor. For example, the occlusion detection system may include a primary light emitter that emits a light for communication toward the medicine flow path and is received at a light detector (e.g., after internal reflection of the light). In addition, the occlusion detection system may include a reference light emitter that emits a light for communication along a different path toward the light detector. As such, a comparison of the detected light signal from the reference light emitter and the detected light signal from the primary light emitter can be employed to calibrate the occlusion detection system to account for changes in environmental conditions.

Third, some embodiments of the infusion pump system may include a reusable controller device that houses the electronic components of the occlusion detection system even though the electronic components of the occlusion sensor system are used to detect characteristics the medicine flow path passing through a removable pump device. As such, sensor signals of the occlusion detection system can be readily communicated to control circuitry of the reusable controller device to determine if an occlusion exists. If so, the user interface of the controller device can be used to promptly alert the user of the problem.

Fourth, some embodiments of the infusion pump system may be configured to be portable, wearable, and (in some circumstances) concealable. For example, a user can conveniently wear the infusion pump system on the user's skin under clothing or can carry the pump device in the user's pocket (or other portable location) while receiving the medicine dispensed from the pump device.

The details of one or more embodiments of the invention are set forth in the accompanying drawings and the description below. Other features, objects, and advantages of the invention will be apparent from the description and drawings, and from the claims.

DESCRIPTION OF DRAWINGS

FIG. **1** is an exploded perspective view of an infusion pump system in accordance with some embodiments.

FIG. **2** is a perspective view of the infusion pump system of FIG. **1** in a detached state.

FIG. **3** is a perspective view of an infusion pump system, in accordance with some embodiments.

FIGS. **4-5** are perspective views of the pump device of FIGS. **1-2** being discarded and the controller device of FIGS. **1-2** being reused with a new pump device.

FIG. **6** is an exploded perspective view of a controller device for an infusion pump system, in accordance with some embodiments.

FIG. **7** is an exploded perspective view of a pump device for an infusion pump system, in accordance with some embodiments.

FIG. **8** is a cross-section view of the cap device and the medicine cartridge of FIG. **1**.

FIG. **9** is a perspective view of an alignment of the cap device and occlusion detection system, in accordance with some embodiments.

FIG. **10** is a cross-sectional perspective view of the alignment shown in FIG. **9**.

FIG. **11** is an exploded view of the cap device, in accordance with some embodiments.

FIGS. **12-14** are cross-sectional views of the cap device and occlusion detection system, in accordance with some embodiments.

FIGS. **15-16** are a flow charts used to detect whether the infusion pump system is in an occluded or non-occluded state, in accordance with some embodiments.

Like reference symbols in the various drawings indicate like elements.

DETAILED DESCRIPTION OF ILLUSTRATIVE EMBODIMENTS

Referring to FIG. **1**, an infusion pump system **10** can include a pump device **100** and a controller device **200** that communicates with the pump device **100**. The pump device **100** in this embodiment includes a housing structure **110** that defines a cavity **116** in which a fluid cartridge **120** can be received. The pump device **100** also can include a cap device **130** to retain the fluid cartridge **120** in the cavity **116** of the housing structure **110**. The pump device **100** can include a drive system that advances a plunger **125** in the fluid cartridge **120** so as to dispense fluid therefrom. As described in more detail below in connection with FIGS. **8-16**, the pump system can include an occlusion detection system **250** that is advantageously configured to self-calibrate in a manner that accounts for changes in environmental conditions, such as ambient temperature, pressure, or the like. As such, the occlusion detection system **250** may provide reliable feedback to a user as to the occluded or non-occluded state of the medicine flow path extending between the fluid cartridge **120** and the infusion site.

In some embodiments, the controller device **200** communicates with the pump device **100** to control the operation of the drive system. When the controller device **200**, the pump device **100** (including the cap device **130**), and the fluid cartridge **120** are assembled together, the user can (in some embodiments) conveniently wear the infusion pump system **10** on the user's skin under clothing, in a pouch clipped at the waist (e.g., similar to a cell phone pouch), or in the user's pocket while receiving the fluid dispensed from the pump device **100**. Optionally, the controller device **200** may be configured as a reusable component that provides electronics and a user interface to control the operation of the pump device **100**. In such circumstances, the pump device **100** can be a disposable component that is disposed of after a single use. For example, as described in more detail below in connection with FIGS. **4-5**, the pump device **100** can be a "one time use" component that is thrown away after the fluid cartridge **120** therein is exhausted. Thereafter, the user can

removably attach a new pump device **100'** (having a new medicine cartridge **120'**) to the reusable controller device **200** for the dispensation of fluid from a new fluid cartridge **120'**. Accordingly, the user is permitted to reuse the controller device **200** (which may include complex or valuable electronics, as well as a rechargeable battery) while disposing of the relatively low-cost pump device **100** after each use. Such a pump system **10** can provide enhanced user safety as a new pump device **100'** (and drive system therein) is employed with each new fluid cartridge **120'**.

Briefly, in use, the pump device **100** is configured to removably attach to the controller device **200** in a manner that provides a secure fitting, an overall compact size, and a reliable electrical connection that is resistant to water migration. For example, as described in more detail below in connection with FIGS. **1-5**, the controller device **200** can include a housing **210** having a number of features that mate with complementary features of the pump housing **110**. In such circumstances, the controller device **200** can removably attach with the pump device **100** in a generally side-by-side configuration. The compact size permits the infusion pump system **10** to be discrete and portable (as described below in connection with FIG. **3**).

Referring again to FIG. **1**, the pump system **10** can be a medical infusion pump system that is configured to controllably dispense a medicine from the cartridge **120**. As such, the fluid cartridge **120** can contain a medicine **126** to be infused into the tissue or vasculature of a targeted individual, such as a human or animal patient. For example, the pump device **100** can be adapted to receive a medicine cartridge **120** in the form of a carpule that is preloaded with insulin or another medicine for use in the treatment of Diabetes (e.g., Byetta®, Symlin®, or others). Such a cartridge **120** may be supplied, for example, by Eli Lilly and Co. of Indianapolis, Ind. Other examples of medicines that can be contained in the fluid cartridge **120** include: pain relief drugs, hormone therapy, blood pressure treatments, anti-emetics, osteoporosis treatments, or other injectable medicines. The fluid cartridge **120** may have other configurations. For example, the fluid cartridge **120** may comprise a reservoir that is integral with the pump housing structure **110** (e.g., the fluid cartridge **120** can be defined by one or more walls of the pump housing structure **110** that surround a plunger to define a reservoir in which the medicine is injected or otherwise received).

In some embodiments, the pump device **100** can include one or more structures that interfere with the removal of the medicine cartridge **120** after the medicine cartridge **120** is inserted into the cavity **116**. For example, the pump housing structure **110** can include one or more retainer wings (not shown in FIG. **1**) that at least partially extend into the cavity **116** to engage a portion of the medicine cartridge **120** when the medicine cartridge **120** is installed therein. Such a configuration may facilitate the "one-time-use" feature of the pump device **100**. In some embodiments, the retainer wings can interfere with attempts to remove the medicine cartridge **120** from the pump device **100**, thus ensuring that the pump device **100** will be discarded along with the medicine cartridge **120** after the medicine cartridge **120** is emptied, expired, or otherwise exhausted. Accordingly, the pump device **100** can operate in a tamper-resistant and safe manner because the pump device **100** can be designed with a predetermined life expectancy (e.g., the "one-time-use" feature in which the pump device is discarded after the medicine cartridge **120** is emptied, expired, or otherwise exhausted).

Still referring to FIG. **1**, the controller device **200** can be removably attached to the pump device **100** so that the two components are mechanically mounted to one another in a fixed relationship. Such a mechanical mounting can form an electrical connection between the removable controller device **200** and the pump device **100**. For example, the controller device **200** can be in electrical communication with a portion of a drive system (not shown in FIG. **1**) of the pump device **100**. As described in more detail below, the pump device **100** can include a drive system that causes controlled dispensation of the medicine or other fluid from the cartridge **120**. In some embodiments, the drive system incrementally advances a piston rod (not shown in FIG. **1**) longitudinally into the cartridge **120** so that the fluid is forced out of an output end **122**. A septum **121** (FIG. **1**) at the output end **122** of the fluid cartridge **120** can be pierced to permit fluid outflow when the cap device **130** is connected to the pump housing structure **110**. For example, the cap device **130** may include a penetration needle that punctures the septum **121** during attachment of the cap device to the housing structure **110**. Thus, when the pump device **100** and the controller device **200** are attached and thereby electrically connected, the controller device **200** communicates electronic control signals via a hardwire-connection (e.g., electrical contacts or the like) to the drive system or other components of the pump device **100**. In response to the electrical control signals from the controller device **200**, the drive system of the pump device **100** causes medicine to incrementally dispense from the medicine cartridge **120**. Power signals, such as signals from the rechargeable battery **245** (refer to FIG. **6**) of the controller device **200** and from the power source **310** (refer to FIG. **7**) of the pump device **100** may also be passed between the controller device **200** and the pump device **100**.

As shown in FIG. **1**, the pump device **100** can include an electrical connector **118** (e.g., having conductive pads, pins, and the like) that is exposed to the controller device **200** and that mates with a complementary electrical connector (refer to connector **218** in FIG. **2**) on the adjacent face of the controller device **200**. The electrical connectors **118** and **218** provide the electrical communication between the control circuitry (refer, for example, to FIG. **6**) housed in the controller device **200** and at least a portion of the drive system or other components of the pump device **100**. For example, in some embodiments, the electrical connectors **118** and **218** can permit the transmission of electrical control signals to the pump device **100** and the reception of feedback signals (e.g., sensor signals) from particular components within the pump device **100**. The electrical connectors **118** and **218** may similarly facilitate transmission of one or more power signals from the rechargeable battery pack **245** to the pump device **100**, where the signals may be used to provide power to components of the pump device **100**, or to transmit one or more power signals from the power source **310** to the controller device, where the signals may be used to charge the rechargeable battery **245** or to power components of the controller device **200**.

Still referring to FIG. **1**, the controller device **200** can include a user interface **220** that permits a user to monitor the operation of the pump device **100**. In some embodiments, the user interface **220** can include a display device **222** and one or more user-selectable buttons (e.g., several buttons **224** are shown in the embodiment of FIG. **1**). The display device **222** can include an active area in which numerals, text, symbols, images, or a combination thereof can be displayed. For example, the display device **222** can be used to communicate a number of settings or menu options for the infusion pump system **10**. In this embodiment, the user may press one or more of the buttons to shuffle through a number of menus or program screens that show particular settings and data (e.g., review data that shows the medicine dispensing rate, the total

amount of medicine dispensed in a given time period, the amount of medicine scheduled to be dispensed at a particular time or date, the approximate amount of medicine remaining in the cartridge **120**, or the like). In some embodiments, the user can adjust the settings or otherwise program the controller device **200** by pressing one or more buttons of the user interface **220**. For example, in embodiments of the infusion pump system **10** configured to dispense insulin, the user may press one or more of the buttons to change the dispensation rate of insulin or to request that a bolus of insulin be dispensed immediately or at a scheduled, later time. In some implementations, the display device **222** may also be used to communicate information regarding remaining battery life.

Accordingly, when the controller device **200** is connected to the pump device **100**, the user can be provided with the opportunity to readily monitor the infusion pump operation by simply viewing the user interface **220** of the controller device **200** connected to the pump device **100**. Such monitoring capabilities may provide comfort to a user who may have urgent questions about the current operation of the pump device **100**. Also, in these embodiments, there may be no need for the user to carry and operate a separate module to monitor the operation of the pump device **100**, thereby simplifying the monitoring process and reducing the number of devices that must be carried by the user. If a need arises in which the user desires to monitor the operation of the pump device **100** or to adjust the settings of the pump system **10** (e.g., to request a bolus amount of medicine), the user can readily operate the user interface **220** of the controller device **200**, which is removably attached to the pump device **100**, without the requirement of locating and operating a separate monitoring module.

Referring now to FIG. **2**, when the infusion pump system **10** operates, the controller device **200** can be removably attached to the pump device **100** in a side-by-side arrangement. For example, the pump device **100** may be moved in a longitudinal direction (e.g., refer to direction **219** in FIG. **4**) toward the controller device **200** until the complementary features connect and secure the separate components in the side-by-side arrangement. The controller device **200** can include a controller housing structure **210** having a number of features that are configured to mate with complementary features of the pump housing structure **110** so as to form a releasable mechanical connection. For example, the pump housing structure **110** can include a barrel **111** that mates with a complementary barrel channel **211** of the controller housing **210**. In various implementations, the pump device **100** and the controller device **200** can be mounted to one another so that the assembled system **10** is resistant to water migration both into the pump housing structure **110** and the controller housing structure **210**. Such a configuration can also provide water-resistant protection for the electrical connection between the pump device **100** and the controller device **200**. Thus, the sensitive internal components in the controller device **200** and the pump device **100** can be reliably protected from water migration if the user encounters water (e.g., rain, incidental splashing, and the like) while using the pump system **10**.

Referring to FIG. **3**, the infusion pump system **10** can be configured to be portable and can be wearable and concealable. For example, a user can conveniently wear the infusion pump system **10** on the user's skin (e.g., skin adhesive) underneath the user's clothing or carry the pump device **100** in the user's pocket (or other portable location) while receiving the medicine dispensed from the pump device **100**. The pump system **10** is shown in FIG. **3** as being held in a user's hand **5** so as to illustrate an exemplary size of the system **10** in accordance with some embodiments. This embodiment of the infusion pump system **10** is compact so that the user can wear the portable infusion pump system **10** (e.g., in the user's pocket, connected to a belt clip, adhered to the user's skin, or the like) without the need for carrying and operating a separate module. In such embodiments, the cap device **130** of the pump device **100** can be configured to mate with an infusion set **146**. In general, the infusion set **146** can be a tubing system that connects the infusion pump system **10** to the tissue or vasculature of the user (e.g., to deliver medicine into the tissue or vasculature under the user's skin). The infusion set **146** can include a flexible tube **147** that extends from the pump device **100** to a subcutaneous cannula **149** that may be retained by a skin adhesive patch (not shown) that secures the subcutaneous cannula **149** to the infusion site. The skin adhesive patch can retain the infusion cannula **149** in fluid communication with the tissue or vasculature of the patient so that the medicine dispensed through the tube **147** passes through the cannula **149** and into the user's body. The cap device **130** can provide fluid communication between the output end **122** (FIG. **1**) of the medicine cartridge **120** and the tube **147** of the infusion set **146**.

In some embodiments, the infusion pump system **10** can be pocket-sized so that the pump device **100** and controller device **200** can be worn in the user's pocket or in another portion of the user's clothing. In some circumstances, the user may desire to wear the pump system **10** in a more discrete manner. Accordingly, the user can pass the tube **147** from the pocket, under the user's clothing, and to the infusion site where the adhesive patch can be positioned. As such, the pump system **10** can be used to deliver medicine to the tissues or vasculature of the user in a portable, concealable, and discrete manner.

In some embodiments, the infusion pump system **10** can be configured to adhere to the user's skin directly at the location in which the skin is penetrated for medicine infusion. For example, a rear surface **102** (FIG. **2**) of the pump device **100** can include a skin adhesive patch so that the pump device **100** can be physically adhered to the skin of the user at a particular location. In these embodiments, the cap device **130** can have a configuration in which medicine passes directly from the cap device **130** into an infusion cannula **149** that is penetrated into the user's skin. In some examples, the user can temporarily detach the controller device **200** (while the pump device **100** remains adhered to the skin) so as to view and interact with the user interface **220**.

Referring now to FIGS. **4-5**, the infusion pump system **10** can be operated such that the pump device **100** is a disposable, non-reusable component while the controller device **200** is a reusable component. In these circumstances, the pump device **100** may be configured as a "one-time-use" device that is discarded after the medicine cartridge is emptied, expired, or otherwise exhausted. Thus, in some embodiments, the pump device **100** can be designed to have an expected operational life of about 1 day to about 30 days, about 1 day to about 20 days, about 1 to about 14 days, or about 1 day to about 7 days—depending on the volume of medicine in the cartridge **120**, the dispensation patterns that are selected for the individual user, and other factors. For example, a medicine cartridge **120** containing insulin can have an expected usage life of about 7 days after the cartridge is removed from a refrigerated state and the septum **121** is punctured. In some circumstances, the dispensation pattern selected by the user can cause the insulin to be emptied from the medicine cartridge **120** before the 7-day period. If the insulin is not emptied from the medicine cartridge **120** after the 7-day period, the remaining insulin can become expired sometime thereafter. In either

case, the pump device **100** and the medicine cartridge **120** therein can be collectively discarded after exhaustion of the medicine cartridge **120** (e.g., after being emptied, expired, or otherwise not available for use).

The controller device **200**, however, may be reused with subsequent new pump devices **100'** and new medicine cartridges **120'**. As such, the control circuitry, the user interface components, the rechargeable battery pack **245**, and other components that may have relatively higher manufacturing costs can be reused over a longer period of time. For example, in some embodiments, the controller device **200** can be designed to have an expected operational life of about 1 year to about 7 years, about 2 years to about 6 years, or about 3 years to about 5 years—depending on a number of factors including the usage conditions for the individual user. Accordingly, the user can be permitted to reuse the controller device **200** (which can include complex or valuable electronics, and a rechargeable battery pack) while disposing of the relatively low-cost pump device **100** after each use. Such a pump system **10** can provide enhanced user safety as a new pump device **100'** (and drive system therein) is employed with each new medicine cartridge **120'**.

Referring to FIGS. **4-5**, the same controller device **200** can be reused with a new pump device **100'** having a new medicine cartridge **120'** retained therein, and the previously used pump device **100**, including the exhausted medicine cartridge, can be discarded in a discard bin **20**. The new pump device **100'** (FIG. **4**) can have a similar appearance, form factor, and operation as the previously used pump device **100**, and thus the new pump device **100'** can be readily attached to the controller device **200** for controlled dispensation of medicine from the new medicine cartridge **120'**. In some embodiments, the user can prepare the new pump device **100'** for use with the controller device **200**. For example, the user may insert the new medicine cartridge **120'** in the cavity **116** of the new pump device **100'** and then join the cap device **130** to the pump housing to retain the new medicine cartridge **120'** therein (refer, for example, to FIG. **1**). Although the tubing **147** of the infusion set **146** is not shown in FIG. **4**, it should be understood that the tubing **147** can be attached to the cap device **130** prior to the cap device **130** being joined with the housing **110**. For example, a new infusion set **146** can be connected to the cap device **130** so that the tubing **147** can be primed (e.g., a selected function of the pump device **100** controlled by the controller device **200**) before attaching the cannula's adhesive patch to the user's skin. As shown in FIG. **4**, the new medicine cartridge **120'** may be filled with medicine such that the plunger **125** is not viewable through the barrel **111**.

The new pump device **100'** can be removably attached to the controller device **200** to assemble into the infusion pump system **10** for delivery of medicine to the user. As previously described, the guided motion in the longitudinal direction **219** provides the user with a convenient "one-movement" process to attach the pump device **100'** and the controller device **200**. For example, the user can readily slide the pump device **100'** and the controller device **200** toward one another in a single movement (e.g., in the longitudinal direction **219**) that causes both a physical connection and an electrical connection. Thus, the infusion pump system **10** can permit users to readily join the pump device **100'** and the controller device **200** without compound or otherwise difficult hand movements—a feature that can be particularly beneficial to child users or to elderly users.

Referring now to FIG. **6**, the controller device **200** (shown in an exploded view) houses a number of components that can be reused with a series of successive pump devices **100**. In particular, the controller device **200** can include controller circuitry **240** and a rechargeable battery pack **245**, each arranged in the controller housing **210**. As described above, rechargeable battery pack **245** may provide electrical energy to components of controller circuitry **240**, other components of the controller device (e.g., a display device **222** and other user interface components, sensors, or the like), or to components of the pump device **100**. Controller circuitry **240** may be configured to communicate control or power signals to the drive system of the pump device **100**, or to receive power or feedback signals from the pump device **100**.

Furthermore, the control circuitry **240** may include one or more dedicated memory devices **242** that store executable software instructions for a processor **243** communicatively coupled to the control circuitry **240**. The control circuitry **240** may include other components, such as sensors, that are electrically connected to the main processor board **242**. For example, at least a portion of the occlusion detection system **250** can be electrically connected to the main processor board **242** via a flexible circuit substrate or one or more wires, as described in more detail below in connection with FIG. **9**.

Still referring to FIG. **6**, the user interface **220** of the controller device **200** can include input components and/or output components that are electrically connected to the controller circuitry **240**. For example, the user interface **220** can include the display device **222** having an active area that outputs information to a user and buttons **224** that the user can use to provide input. Here, the display device **222** can be used to communicate a number of settings or menu options for the infusion pump system **10**. In some embodiments, the controller circuitry **240** can receive input commands from a user's button selections and thereby cause the display device **222** to output a number of menus or program screens that show particular settings and data (e.g., review data that shows the medicine dispensing rate, the total amount of medicine dispensed in a given time period, the amount of medicine scheduled to be dispensed at a particular time or date, the approximate amount of medicine remaining the cartridge **120**, the amount of battery life remaining, or the like). The controller circuitry **240** can be programmable to cause the controller circuitry **240** to change any one of a number of settings for the infusion pump system **10**. For example, the user may provide one or more instructions to adjust a number of settings for the operation of the infusion pump system **10**. Such settings may be stored in one or more memory devices arranged in the controller circuitry **240**.

In some optional embodiments, the controller circuitry **240** can include a cable connector (e.g., a USB connection port or another data cable port) that is accessible on an external portion of the controller housing **210**. As such, a cable can be connected to the controller circuitry **240** to upload data or program settings to the controller circuitry or to download data from the controller circuitry. For example, historical data of medicine delivery can be downloaded from the controller circuitry **240** (via the cable connector) to a computer system of a physician or a user for purposes of analysis and program adjustments. Optionally, the data cable can also provide recharging power.

Referring now to FIG. **7**, the pump device **100** can include a drive system **300** that is controlled by the controller device **200**. In this embodiment, the drive system **300** can incrementally dispense fluid in a controlled manner from cartridge **120** inserted into the pump device **100**. Also, the pump device **100** may include a connector circuit **318** to facilitate the transfer of signals to and from the electrical connector **118**. In some implementations, the connector circuit **318** in the pump device **100** may include a memory device that can store data

regarding the pump device **100** and its operational history. As previously described, the electrical connector **118** of the pump device **100** can mate with the connector **218** (FIG. **2**) of the controller device **200** so that electrical communication can occur between the pump device **100** and the controller device **200**. In some embodiments, the connector circuit **318** can operate as a passageway to transmit electrical control signals from the controller circuitry **240** of the controller device **200** to the drive system **300**. The connector circuit **318** can also operate as a passageway for the electrical power from a power source **310** housed in the pump device **300** to pass to the controller device **200** for recharging of the rechargeable battery **245**. Furthermore, the connector circuit **318** can operate as a passageway for feedback signals from the drive system **300** to the controller circuitry **240** of the controller device **200**.

In this embodiment, the pump device **100** houses the drive system **300** and the power source **310**. For example, the power source **310** may comprise an alkaline battery cell, such as a 1.5 Volt "AAA" alkaline battery cell, which is contained in a dedicated space of the pump housing structure **110**. The power source **310** may be capable of transmitting electrical energy to the controller device **200** when the pump device **100** is attached to the controller device **200**, via connectors **118** and **218** as described above. For example, the power source **310** may be used to charge the rechargeable battery pack **245** when the pump device **100** is attached to the controller device **200**. In some embodiments, the power source **310** is used to provide energy to the drive system **300** of the pump device **100**, and also to electronic components of the controller device **200**. In particular embodiments, the power source **310** may provide the energy to power all aspects of the infusion pump system **10**. In some alternative embodiments, the rechargeable battery **245** housed in the controller **200** may provide the energy to power all aspects of the infusion pump system **10**. In other embodiments, the rechargeable battery **245** and the power source **310** may each be responsible for powering particular aspects of the infusion pump system **10**. In further embodiments, the rechargeable battery **245** may provide the energy to supplement the energy provided by the power source **310** to power aspects of the infusion pump system.

Still referring to FIG. **7**, in some embodiment, the drive system **300** may include a number of components, such as an electrically powered actuator (e.g., reversible motor **320** or the like), a drive wheel **360**, a bearing **365**, a flexible piston rod **370**, a piston rod guide **363**, and a plunger engagement device **375**. In this embodiment, the reversible motor **320** drives a gear system to cause the rotation of the drive wheel **360** that is coupled with bearing **365**. The drive wheel **360** may include a central aperture with an internal thread pattern, which mates with an external thread pattern on the flexible piston rod **370**. The interface of the threaded portions of the drive wheel **360** and flexible piston rod **370** may be used to transmit force from the drive wheel to the piston rod **370**. Accordingly, in the embodiment of FIG. **7**, the drive wheel **360** is the driver while the flexible piston rod **370** is the driven member. As further described below, the rotation of the drive wheel **360** can drive the flexible piston rod **370** forward in a linear longitudinal direction.

Referring now to FIGS. **8-16**, some embodiments of the occlusion detection system **250** can be configured to self-calibrate so as to reliably perform even when the pump system **10** is exposed to significant changes in environmental conditions, such as changes to the ambient temperature, pressure, or the like. In such circumstances, the occlusion detection system **250** can be used to provide reliable feedback to a user as to the occluded or non-occluded state of the medicine flow path. Further, the user interface **220** of the controller device **200** can be used to communicate an alarm to the user if an occlusion exists.

Referring to FIG. **8**, the cap device **130** can have a multi-piece construction that provides a flow path from the medicine container **120** to the infusion set tubing **147** (e.g., via an output port **139**). At least a portion of the flow path through the cap device **130** may be monitored by the occlusion detection system **250** to determine if an occlusion exists downstream of the cap device **130** (e.g., if a kink or clog exists in the infusion set tubing **147** of cannula **149**). The multi-piece construction of the cap device **130** can facilitate proper alignment of the cap device **130** and proper engagement with the medicine cartridge **120** during attachment of the cap device **130** to the pump housing **110**. For example, during attachment of the cap device **130** to the pump housing, a needle penetrator **133** attached to a portion of the cap device can be advanced toward the septum of the medicine cartridge **120** to pierce the septum and open a fluid flow path. The flow path for the medicine that is dispensed from the medicine cartridge **120** can pass through the needle penetrator **133**, through a fluid channel **260** (described below), through the infusion set tubing **147**, and to the user.

The fluid channel **260** arranged in the cap device **130** may include a secondary channel **262** that extends to a flexible member **265**. In this embodiment, one side of the flexible membrane **265** is exposed to the fluid channel **260** (via the secondary channel **262**) while the opposite side of the flexible membrane **265** is adjacent to an air cavity **267** (also shown in FIGS. **12-14**), which provides a volume into which the flexible membrane **265** can expand as pressure rises in the fluid channel **260**. The flexible membrane **265** may comprise a flexible polymer material that bulges or otherwise deforms as the fluid pressure in the flow channel **260** rises and is preferably composed of silicon. As such, the flexible membrane **265** can flex into the air cavity **267** when the fluid pressure rises due to an occlusion in the flow path downstream of the fluid channel **260** (illustrated in reference to FIGS. **12-14**).

Referring to FIG. **9**, the occlusion detection system **250** may include a number of components that are housed in the controller device **200**. For example, the occlusion detection system **250** may include one or more light emitters and a light sensor arranged on the sensor circuit **252** that is housed by the controller device **200**, thereby permitting these components to be reused along with the controller device (while the relatively low cost components in the pump device **100** are discarded after the "one time use" of the pump device **100**). In a preferred embodiment, the sensor circuit **252** includes a primary light emitter **253**, a reference light emitter **255**, and a light sensor **258**.

The sensor circuit **252** can be arranged so that the cap device **130** is aligned with the light emitters **253**, **255** and the light sensor **258** when the pump device **100** is attached to the controller device **200**. It should be understood that the pump housing **110** and the controller housing **210** have been removed from FIG. **9** for purposes of showing the relative position of the sensor circuit **252** (in the controller device **200** as shown in FIGS. **2** and **4**) and the cap device **130** (attached to the pump housing **110** as shown in FIG. **2**).

The sensor circuit **252** can be connected to the control circuitry **240** of the controller device **200** (FIG. **6**) via a flexible circuit substrate or one or more wires. In a preferred embodiment, the sensor circuit **252** connects with the main processor board **242** via the flexible circuit substrate illustrated in FIG. **6**. As such, the control circuitry **240** can receive sensor signals and employ detection software stored in one or

more memory devices **242** to determine if an occlusion exists. If the sensor signals from the occlusion detection system **250** indicate that an occlusion exists in the fluid flow path, the controller device **200** can trigger an alert to inform the user. The alert may include a visual or audible alarm communicated via the user interface **220** of the controller device **200**.

The light collector **256** can be made of any reflective material, preferably polished aluminum, and is designed to collect light from both the reference light emitter **255** and the primary light emitter **253**. For example, apertures are advantageously constructed in the light collector **256** to allow light to reach the light sensor **258** from specific directions corresponding to light originating from the reference light emitter **255** and from the primary light emitter **253** (described below in connection with FIGS. **12-14**).

In some embodiments, the reference light emitter **255** can provide a reference light reading at the sensor **258**, which can be advantageously compared to a light reading from the primary light emitter **253** for purposes of determining when a reduced light reading from the main emitter **253** is caused by a buildup of fluid pressure in the fluid channel **260** (e.g., from an occlusion in the infusion set tubing **147**) or is caused by some other reason not related to the presence of an occlusion (e.g., environmental conditions such as ambient temperature). For example, in some embodiments, the amount of light emitted from the primary emitter **253** begins to degrade or otherwise changes with fluctuations in ambient temperature and ambient light condition. If the control circuitry was configured to rely upon the light sensor readings detected by the light sensor **258** from the primary emitter **253** alone, such reductions in the amount of the light readings from the primary light emitter **253** would possibly induce false occlusion warnings (e.g., occlusion alerts where in fact the suboptimal temperatures are responsible for the reduced light readings and no occlusion is present in the infusion set tubing **147**). In this embodiment, each of the primary emitter **253** and the reference light emitter **255** are substantially equally affected by the fluctuations in ambient temperature and ambient light condition. Accordingly, a comparison of the amount of the light received from the primary light emitter **253** with the amount of the light received from the reference light emitter **255** (rather than an absolute light measurement from the primary light emitter **253** alone) can be employed to substantially reduce or eliminate the number of false occlusion warnings.

Referring to FIG. **10**, the sensor circuit **252** can be arranged so that the flexible membrane **265** and air gap **267** in the cap device **130** are aligned with the primary light emitter **253** and the light sensor **258** when the pump device **100** is attached to the controller device **200** (FIG. **2**). Thus, when the infusion pump system **10** is preparing to dispense an incremental dosage of medicine, the primary light emitter **253** in the controller device **200** can direct light toward the flexible membrane **265** and air gap **267** in the cap device **130**, and the light sensor **258** can receive light reflected from portions of the cap device **130**. A cross-section through the cap device **130** and the controller device **200** illustrates one example of the alignment (although, here, the pump housing **110** and the controller housing **210** have been removed from FIG. **10** for purposes of better illustrating the alignment). It should be understood from the description herein that other alignment configurations can be implemented so that the light sensor **258** in the reusable controller device **200** is able to detect changes to fluid flow conditions in the pump device **100**.

In the depicted embodiment, the sensor circuit **252** is arranged to at least partially extend to the barrel channel **211** (FIG. **2**) of the controller device **200** so that the primary light emitter **253** and the light sensor **258** are positioned adjacent to the cap device **130**. The light from the primary light emitter **253** can pass through one or more portions of the cap device **130** during its travel toward the flexible membrane **265** and air cavity **267** (shown in FIGS. **12-14**). Accordingly, some portions of the cap device **130** may comprise a generally transparent material to permit light transmission therethrough. For example, the cap device may comprise a light transmissive member **254** that acts to transmit light from the primary light emitter **253** toward the flexible membrane **265** and air cavity **267**, and in some cases, further acts to transmit reflected light toward the light sensor **258**. Also, some portions of the controller housing **210** (FIG. **2**) may include generally transparent material to permit light transmission therethrough. For example, in this embodiment, a first window component **136** of the controller housing **210** can include a generally transparent polymer material, which is positioned adjacent to the primary light emitter **253** so that the light from the primary emitter **253** is transmitted to the light transmissive member **254** of the cap device **130**. Also, in this embodiment, a second window component **138** of the controller housing **210** is positioned adjacent to the light collector **256** and the light sensor **258**. As such, when the pump device **100** is attached to the controller device **200**, the second window component **138** is positioned between the light transmissive member **254** and the light sensor **258**. Preferably, the remaining portion of the controller housing **210** that surrounds the reference light emitter **255** is generally opaque so that the light emitted from the reference light emitter **255** is prevented from passing to the light transmissive member **254** of the cap device **130**. Such a construction may prevent or reduce the likelihood of inaccurate readings caused by light from the reference light emitter **255** interfering with the light emitted by the primary light emitter **253**.

Still referring to FIG. **10**, the internal light transmissive member **254** can be configured to receive light from the primary light emitter **253** and transmit at least a portion of that light toward the flexible membrane **265** and air cavity **267**. In this embodiment, the internal light transmissive member **254** comprises a generally transparent polymer material that is capable of light transmission. As described in more detail below, the light that is transmitted in the light transmissive member **254** toward the fluid channel **260** can (in some circumstances) reflect from the interface where the internal light transmissive member **254** meets the air cavity **267**. This reflected light can be further transmitted through the internal light transmissive member **254** to the light sensor **258**.

Referring now to FIG. **11**, the internal transmissive member **254** can be affixed to the remaining components of the cap device **130** using a bonding material **266**, such as an adhesive film or glue. The flexible membrane **265** is positioned to form a seal between the fluid channel **262** and light transmissive member **254**. That is, once the flexible membrane **265** is assembled into the cap device **130**, the flexible membrane **265** deforms in response to a buildup of fluid pressure in the fluid path **260** (which is communicated via the secondary channel **262**), but does not allow fluid in the fluid channel **260** to escape pass the membrane **265** into the air cavity **267** or otherwise interfere with other components of the pump device **100** or the controller device **200**. This deformation of the flexible membrane **265** may change the size of the air cavity **267** (shown in FIGS. **12-14**), which advantageously allows the light sensor to detect a change in the amount of the light emitted by the primary light emitter **253** indicating a possible occlusion of medicine flow path through the infusion set tubing **147** (FIGS. **3** and **8**) which may prevent medicine from being delivered to the user.

Referring now to FIGS. **12-14**, the occlusion detection system **250** can be used to detect when an occlusion exists in the flow path from the pump device **100** to the user. For example, when an occlusion occurs in the infusion set tubing **146** or the infusion set tubing **147** (FIGS. **3** and **8**), the delivery of medicine from the infusion pump system **10** to the user can be stopped or otherwise limited. If the user is unaware of the occlusion, the user may be deprived of the intended dosages of medicine from the infusion pump device for a period of time. Accordingly, the occlusion detection system **250** can be used to detect when such occlusions occur in the flow path to the user, and the controller device **200** can thereafter alert the user of the occlusion when particular conditions are met. The user may then inspect the pump device **100** or the infusion set **146** to eliminate the occlusion.

As shown in FIGS. **12-13**, when no substantial occlusion exists in the flow path, the medicine can be dispensed under normal operating conditions from the medicine cartridge **120**, through the cap device **130**, and into the infusion tubing **147**. In these normal operating conditions, the fluid pressure of the medicine passing through the cap device **130** may be below a selected threshold value. As such, the flexible membrane **265** that is adjacent to the fluid channel **260** is not substantially deformed (e.g., the membrane **265** does not flex downwardly into the air cavity **267** to abut the internal light transmissive member **254**).

Referring to FIG. **12**, in some embodiments, the occlusion sensor **250** may operate by activating the reference light emitter **255** in isolation from the primary light emitter **253**. When the reference light emitter **255** is activated, the light is received by the light collector **256** and directed toward the light sensor **258** without passing through the light transmissive member **254** or any other portion of the cap device **130**. For example, as shown in FIG. **12**, at least a portion of the light from the reference emitter **255** (e.g., a wide-angle LED emitter in this embodiment) reflects off a surface of the light collector **256** and is received by the light sensor **258**. As previously described, the generally opaque portion of the controller housing **210** (FIG. **2**) may optionally prevent the light from the reference emitter **255** from passing outside the controller housing **210**. Here, because the reference light emitter **255** does not transmit light through the light transmissive member **254**, the amount of light transmitted by the reference light emitter **255** and received by the light sensor **258** is generally unaffected by a buildup of fluid pressure in the fluid channel **260** (as will be described in more detail in reference to FIGS. **13-14**).

In other words, the amount of light emitted by the reference emitter **255** and received by the light sensor **258** does not fluctuate according to fluid pressure but may fluctuate according to other environmental factors, such as ambient temperature (and it should be understood that primary light emitter **253** is similarly affected by these same environmental factors). This configuration can be employed to aid in the detection of an occlusion that accounts for changes in environmental factors affecting the primary light emitter **253**. For example, when the pump device **10** is operating in regions having lower ambient temperatures, both the reference light emitter **255** and the primary light emitter **253** will have reduced light outputs. In those circumstances, the occlusion detection system **250** can use the reduction in the amount of light from the reference light emitter **255** to account for the reduction in the amount of light from the primary light emitter **253**. In other circumstances in which the light sensor **258** receives a reduced light signal only from the primary light emitter **253** while the light sensor **258** receive a normal light signal from the reference light emitter **255**, then there is a greater likelihood of the presence of an occlusion and the user may be warned accordingly.

Referring to FIG. **13**, when the medicine flow path is in a non-occluded state under normal operating circumstances, the light from the light emitter **253** can be reflected at the interface where the internal light transmissive member **254** meets the air cavity **267**. In some embodiments, this light reflection may occur due to total internal reflection that the interface. Total internal reflection can occur in some circumstances when light passes through a first medium (e.g., the internal light transmissive member **254**) and strikes an interface between the first medium and a second medium (e.g., the air cavity **267**) at an angle greater than the critical angle. If the refractive index of the second medium (e.g., the air cavity **267**) is lower than refractive index of the first medium (e.g., the internal light transmissive member **254**), the light may undergo total internal reflection within the first medium.

For example, as shown in FIG. **13**, the light emitter **253** can be an infrared light emitter that is directed toward the internal light transmissive member **254**. The infrared light passes through the generally transparent first window **136** (shown in FIG. **10**) and then transmits through the light transmissive member **254**. In some embodiments, the surface of the light transmissive member **254** may be curved and may operate as a focusing lens that directs the infrared light toward the air cavity **267** proximate to the fluid channel **260**, although a non-curved surface is shown for the embodiments of FIGS. **12-14**.

Referring still to FIG. **13**, when the medicine is dispensed under normal operating conditions, the flexible membrane **265** does not flex downwardly into the air cavity **267** to abut the internal light transmissive member **254**. Accordingly, the infrared light passing through the internal light transmissive member **254** reflects at the interface where the internal light transmissive member **254** meets the air cavity **267**. This reflected light continues through the internal light transmissive member **254** toward the light sensor **258**. In this embodiment, the reflected light transmitted through the light transmissive member **254** passes through the second window **138** (shown in FIG. **10**) and is subsequently received by the light collector **256** (described in reference to FIG. **9**) and directed toward the light sensor **258**. The light sensor **258** may comprise an infrared photo detector that is capable of converting the receipt of infrared light into electrical signals. These electrical signals from the light sensor **258** can be transmitted via the sensor circuit **252** to the control circuitry **240** (FIG. **6**) for processing to determine if an occlusion alarm should be provided to the user.

Referring to FIG. **14**, when an occlusion exists in the flow path, the fluid pressure of the medicine passing through the cap device **130** may rise to a level above the threshold value. For example, if pump device **100** attempts to dispense another incremental dosage of medicine when the infusion set tubing **147** is clogged or kinked, the fluid pressure upstream of the occlusion (e.g., in the medicine cartridge **120** and in the cap device **130**) may be increased. In these circumstances, the flexible membrane **265** that is in fluid communication with the fluid channel **260** may be substantially deformed (e.g., the membrane **265** will flex downwardly into the air cavity **267** to abut the internal light transmissive member **254**.)

The interface where the light transmissive member **254** meets the flexible membrane **265** (FIG. **14**) provides different optical results than the previously described interface where the internal light transmissive member **254** meets the air cavity (FIG. **13**). In particular, the amount of light from the light emitter **253** that is internally reflected at the interface

where the internal light transmissive member **254** meets the flexible membrane **265** is measurably less (as illustrated by the dotted lines in FIG. **14**). For example, none of the light or some other reduced portion of light from the light emitter **253** is internally reflected. (The light that is not internally reflected at this interface may pass into the medium of flexible membrane **265**, for example.) If any portion of the light is internally reflected, this reduced portion of reflected light continues through the light transmissive member **254** toward the light sensor **258** (e.g., through second window **138** and received by collector **256**). Because amount of light that is internally reflected in the light transmissive member **254** is measurably less, the light sensor **258** can produce detection signals that are different from those described in connection with FIG. **13**. These detection signals may indicate that the fluid pressure in the cap device **130** has risen above a threshold level due to a downstream occlusion. These detection signals from the light sensor **258** (including signals detected from both the reference light emitter **255** and the primary light emitter **253**) can be transmitted via the sensor circuit **252** to the control circuitry **240** (FIG. **6**) for processing to determine if an occlusion alarm should be provided to the user.

FIGS. **15-16** show processes **1500** and **1600**, respectively, that can be performed for purposes of detecting the presence of an occlusion or non-occlusion in the medicine flow path to the pump user. In some embodiments, one or more of the steps described in reference to FIGS. **15-16** may be performed as part of another process. For example, the processes **1500** or **1600** may be performed when the pump device **100** is removably attached to the control device **200** to determine if the pump device **100** and control device **200** are correctly joined. Such a determination may occur in a number of circumstances, including when the pump device **100** and control device **200** are initially assembled after manufacture, or when a user discards a used pump device **100** and removably attaches a new pump device **100'** (FIGS. **4-5**). That is, the depicted processes **1500** or **1600** can be used to ensure that the cap device **130** is properly aligned with the occlusion detection system **250** (e.g., as shown in FIG. **9**). In addition, processes **1500** or **1600** may be performed when a user manually clears an error message presented to the user by the control device **200**. For example, by interacting with the user interface **220**, the display device **222** and the one or more user-selectable buttons **224** (FIG. **1**), the user can cancel an occlusion alarm and the control circuitry **240** may execute processes **1500** or **1600** in response. Also, in a preferred embodiment, processes **1500** or **1600** may be performed prior to each dispensation of medicine to the user to ensure that there are no occlusions in the medicine flow path to the pump user.

Furthermore, in a preferred embodiment, processes **1500** or **1600** may be performed initially to establish baseline light values used in subsequent executions of processes **1500** or **1600**. For example, when the pump device **100** and control device **200** are removably attached or when a user cancels an occlusion alarm (e.g., displayed on displayed device **220**), processes **1500** or **1600** may be performed to establish baseline values of light emitted by both the wide-angle reference light emitter **255** and the primary light emitter **253**. These baseline values can be stored in one or more memory devices (e.g., on the circuit board **242**) by the control circuitry **240** and can be used to determine the presence or absence of an occlusion. For example, if the value corresponding to the light emitted by the primary light emitter **253** is substantially less than the primary light emitter baseline value, an occlusion may exist if the value corresponding to the light emitted by the wide-angle reference light emitter **255** is substantially similar to the wide-angle reference light emitter baseline value. It should be understood that the processes **1500** and **1600** are illustrative of a preferred embodiment. As such, steps described may be performed in orders other than the one described herein.

Referring now to FIG. **15**, some embodiments for the process **1500** for detecting the presence of an occlusion may include steps of activating the reference emitter **155** in isolation from the primary emitter **153**. For example, as shown in the dashed box **1510**, the control circuitry **240** may activate the reference light emitter **255** to emit light. This emitted light reflects off of the interior surface of the light collector **256** and is received by the light sensor **258**. As previously described, the light collector **256** may include a polished interior surface that can redirect the light emitted by the wide-angle light emitter **255** onto the detecting surface of the light sensor **258**. From there, the light sensor **258** can generate an electrical signal corresponding to the received light emission and these electrical signals can be used to determine the amount of emitted light. Optionally, as will be described in reference to FIG. **16**, the step shown by dashed box **1510** may be repeatedly performed a number of times to advantageously reduce the effects of outlier sensor signals by implementing an averaging determination to obtain a more accurate measurement of the light emitted from the light emitter **255**.

Still referring to FIG. **15**, the process **1500** may include a step shown by dashed box **1520** in which the control circuitry **240** waits a predetermined period of time before activating the primary light emitter **253**. For example, the control circuitry **240** may delay for about 0.1 seconds to about 0.9 seconds before activating the primary light emitter **253** (as illustrated by dashed box **1530**). Optionally, during the delay period the control circuitry **240** may present an error message on the display device **222**, alerting the user to the existence of an operating error. For example, a misalignment of the reference light emitter **255** with the cap device **130** may be detected when a baseline value is below some predetermined threshold. As shown in the dashed box **1530**, the control circuitry **240** may then activate the primary light emitter **253**. When the medicine flow path is in an non-occluded state, the emitted light travels through the light transmissive member **254** (FIGS. **13-14**) and is reflected toward the light sensor **258**. As previously described, the reflected light may pass through the light transmissive member **254**, and some or all of the light may reflect from the interface where the internal light transmissive member **254** meets the air cavity **267** (FIG. **10**). Then, the reflected light may pass through the second window **138** (FIG. **9**), the light collector **256** (FIG. **9**), and reach the light sensor **258**. As described in reference to FIGS. **13-14**, the amount of light reaching the light sensor **258** may be indicative of the presence or absence of an occlusion. For example, in some operational circumstances, a reduced electrical signal (relative to previously received electrical signals) received by the control circuitry **240** may indicate the presence of an occlusion or the presence of suboptimal ambient temperature. Conversely, in some operational circumstance, an electrical signal similar to previously received electrical signals (e.g., determined according to multiple executions of processes **1500** or **1600**), may indicate the absence of an occlusion or the presence of optimal ambient temperature.

Still referring to FIG. **15**, as shown by dashed box **1540**, the control circuitry **240** can wait a predetermined period of time. For example, the control circuitry **240** may wait on the order of about 0.1 seconds to about 0.9 seconds before activating the drive system **300** of the pump device **100** to dispense the next dosage of medicine. Optionally, in this embodiment, during the delay period the control circuitry **240** determines

the average light emitted by the primary light emitter **253** corresponding to the one or more electrical signals received by the control circuitry **240** as communicated by the light sensor **258**. In addition, during the delay period the control circuitry **240** may determine the presence or absence of an occlusion by comparing the light detected from the primary light emitter **253** to the light detected from the reference light emitter **255**. In response to the determination of a possible occlusion, the control circuitry **240** may activate the control device **200** to display an alert message on the display device **222** while foregoing the next incremental dosage of medicine.

Referring now to FIG. **16**, the control circuitry **240** may implement a process **1600** to determine whether the medicine flow path is in an occluded or non-occluded state. The process **1600** may be at least partially implemented in an occlusion detection software algorithm that is stored on a memory device and executed by a processor of the control circuitry. In this embodiment, the control circuitry **240** may implement a first iterative step shown by box **1605** so to activate the wide-angle reference light emitter **255** to turn on in step **1602**. For example, because the control circuitry **240** is in electrical communication with the reference light emitter **255**, the control circuitry **240** can generate an electrical signal that when received by the wide-angle reference light emitter **255** causes the wide-angle light emitter **255** to emit light. In addition, the absence of the electrical signal may cause the reference light emitter **255** to deactivate.

In a step shown by box **1604**, the control circuitry **240** detects a signal corresponding to the light emitted by the reference light emitter **255** and received by the light sensor **258**. For example, light transmitted from the reference light emitter **255** may reflect off of the interior surface of the light collector **256** and interact with the light sensor **258**. As described in more detail above, the light sensor **258** can generate an electrical signal corresponding to the received light. Because the control circuitry **240** is in electrical communication with the light sensor **258**, the control circuitry **240** detects the signal corresponding to the light emitted by the wide-angle reference light emitter **255** when the control circuitry **240** receives the electrical signal from the light sensor **258**. In a preferred embodiment, each of the detected signals corresponding to light emitted by the reference light emitter **255** is a floating point value within the range of [0-1] and is stored on one more dedicated memory devices included in the control circuitry **240**.

In a decision shown by step **1606**, the control circuitry **240** determines whether a minimum number of light samples transmitted by the wide-angle light emitter **255** has been received. For example, in a preferred embodiment, the control circuitry **240** determines whether sixteen iterations of activating the reference emitter **255** and detecting the corresponding sixteen electrical signals from the light sensor **258** have been completed. If the minimum number of light samples has not been received, than the control circuitry **240** may instruct the reference light emitter **255** to activate again, repeating the steps included in the first iterative step shown by box **1605**. In this embodiment, the sixteen iterations can be consecutive performed in a period of 0.5 seconds or less.

Once the minimum number of light samples has been received (e.g., sixteen in this embodiment), the control circuitry **240** may perform operation **1612** to determine an average detected value of the reference light emitter samples received. For example, in a preferred embodiment, because the control circuitry **240** receives sixteen light samples from the reference light emitter **255**, the sixteen light samples are added together and the total divided by sixteen to determine the average detected value of the wide-angle reference samples received. In a preferred embodiment, the determined average value corresponding to light transmitted by the reference light emitter **255** is a floating point value within the range of [0-1] and is stored on one or more dedicated memory devices included in the control circuitry **240**.

In a second iterative step shown by box **1620**, the control circuitry **240** activates the primary light emitter **253** as shown in a step **1614**. For example, because the control circuitry **240** is in electrical communication with the primary light emitter **253**, the control circuitry **240** can generate an electrical signal that when received by the primary light emitter **253** activates the primary light emitter **253** to emit light. In addition, the absence of the electrical signal may instruct the primary light emitter **253** to deactivate.

In a step **1616**, the control circuitry **240** can detect a signal corresponding to the light emitted by the primary light emitter **253** and received at the light sensor **258**. For example, the light transmitted from the primary light emitter **253** that passes through the light transmissive member **254**, may be reflected by the interface between the light transmissive member **254** and the air cavity **267** toward the light sensor **258**. As described in more detail above, the light sensor **258** can generate an electrical signal corresponding to the received light. Because the control circuitry **240** is in electrical communication with the light sensor **258**, the control circuitry **240** detects the signal corresponding to the light emitted by the primary light emitter **253** when the control circuitry **240** receives the electrical signal from the light sensor **258**. In a preferred embodiment, each of the detected signals corresponding to the light emitted by the primary light emitter **253** is a floating point value within the range of [0-1] and is stored on one more dedicated memory devices included in the control circuitry **240**.

Still referring to FIG. **16**, the process may continue to a decision shown by box **1618**, in which the control circuitry **240** determines whether a minimum number of light samples transmitted by the primary light emitter **253** has been received. For example, in a preferred embodiment, the control circuitry **240** determines whether sixteen iterations of activating the primary emitter **253** and detecting the corresponding sixteen electrical signals from the light sensor **258** have been completed. If the minimum number of light samples has not been received, than the control circuitry **240** may activate the primary light emitter **253** again, thereby repeating the steps included in the second iterative step shown by box **1620**.

Once the minimum number of light samples has been received, in a step shown by box **1622**, the control circuitry **240** determines an average detected value of the primary light emitter samples received. For example, in a preferred embodiment, because the control circuitry **240** receives 16 light samples from the primary light emitter **253**, the 16 light samples are added together and the total divided by 16 to determine the average detected value of the primary light emitter samples received. In a preferred embodiment, the determined average value corresponding to light transmitted by the primary light emitter **253** is a floating point value within the range of [0-1] and is stored on one or more dedicated memory devices included in the control circuitry **240**.

The process **1600** for to determining whether the medicine flow path is in an occluded or non-occluded state may include an operation that compares the detected value of the light emitted by the primary light emitter **253** with the detected value of the light emitted by the reference light emitter **253**. For example, in this embodiment, the step **1624** indicates that the control circuitry **240** compares the average detected value of the light emitted by the primary light emitter **253** (determined by the step shown by box **1622**) with the average

detected value of the light emitted by the wide-angle reference light emitter **253** (determined by the step shown by box **1612**). In one example of this comparison function, the average detected value of the light emitted by the primary light emitter **253** is divided by the average detected value of the light emitted by the wide-angle reference light emitter **255**. Also, in particular embodiments, the resulting comparison value is a floating point value within the range of [0-1] and is stored on one more dedicated memory devices included in the control circuitry **240**.

In an optional step shown by dashed box **1626**, the control circuitry **240** normalized the comparison value determined in the step shown by box **1624**. For example, in a preferred embodiment, the floating point comparison value in the range of [0-1] is multiplied by 100, normalizing the comparison value to an integer value in the range of [0-100].

The process **1600** may use the comparison value as an indicator of whether the medicine flow path is in an occluded or non-occluded state. For example, in this embodiment, the process **1600** includes a step **1628** in which the control circuitry **240** determines if the comparison value (e.g., either of the values determined by the step shown by box **1624** or the normalized comparison value determined in the step shown by box **1626**) is outside a threshold range (e.g., less than or equal to a minimum threshold value, or greater than or equal to a maximum threshold value, or the like).

In particular embodiments, this step **1628** may employ a baseline value, which can be initially calculated when the pump device **100** is initially primed to force medicine through the infusion set tubing **147** (e.g., when there are no blockages or kinks and the medicine is visibly moved out of the tubing **147**). In some cases, the baseline value can be calculated by the control circuitry **240** as a value corresponding to an initial amount of detected light from the primary light emitter **253** during or immediately before the priming operation divided by a value corresponding to a initial amount of light emitted by the reference light emitter **255** during or immediately before the priming operation).

In this embodiment of step **1628**, the normalized comparison value (e.g., from step **1626**) is divided by this previously determined baseline value. In a preferred embodiment, if this comparison is less than or equal to a minimum threshold value (such as 40% in this embodiment), then the comparison is outside the threshold range. In other words, for this particular embodiment, the comparison value is outside the threshold range when:

$(M_D/R_D)/(M_B/R_B)$ is less than or equal to 40%, where

- M_D is the averaged value of the detected light values from the primary light emitter **253** determined in the step shown by box **1612**,
- R_D is the averaged value of the detected light values from the reference light emitter **255** determined in the step shown by box **1622**,
- M_B is the averaged value of the detected baseline values from the primary light emitter **253** (e.g., recorded and stored by the control circuitry **240** during or immediately before the initial priming operation for the pump device), and
- R_B is averaged value of the detected baseline values from the reference light emitter **255** (e.g., recorded and stored by the control circuitry **240** during or immediately before the initial priming operation for the pump device).

It should be understood from the description herein that the minimum threshold value can be a value other than 40%. For example, in other embodiments, the minimum threshold value can be implemented in the occlusion detection software as a value selected from the range of about 10% to about 70%, about 20% to about 60%, and preferably about 30% to about 50%.

Optionally, in some embodiments, the control circuitry **240** stores a set of the most recently calculated comparison values from step **1628**. This set of recent comparison values from step **1628** can be employed by the occlusion detection software of the control circuitry **240** to determine if there is a trend that is indicative of an ongoing occlusion in the medicine flow path. For example, if a plurality of consecutive values from the comparison step **1628** are all less than or equal to the minimum threshold value (such as 40% in this embodiment), occlusion detection software of the control circuitry **240** may determine that an occlusion exists and a user alert should be output. In this particular embodiment, the control circuitry **240** stores at least five of the most recent comparison values from the step **1628**. In such embodiments, when the most recent five comparison values from the step **1628** are outside the threshold range, then the control circuitry **240** will generate an occlusion alarm in a step shown by box **1630**. Alternatively, the control circuitry **240** may not necessarily store a plurality of the most recently calculated comparison values from step **1628**, but instead may generate the occlusion alarm in step **1630** after any one instance of the comparison value from step **1628** are outside the threshold range.

The process **1600** can be performed immediately prior to each drive cycle of the pump device **100**. In such circumstances, the process may proceed to step **1632** in which the pump drive cycle is initiate if the comparison value from step **1628** is not outside the threshold range (or, in a preferred embodiment, if one of the five most recent comparison values is not outside the threshold range). For example, if the comparison step **1628** reveals that $(M_D/R_D)/(M_B/R_B)$ is greater than 40%, this result is an indication that there is no meaningful occlusion in the medicine flow path and the control circuitry **240** may then initiate the pump drive cycle **1632**. When the control circuitry **240** initiates the pump drive cycle in step **1632** (e.g., in accordance with a previously determined basal dosage schedule or a requested bolus dosage), the pump drive system **300** is activated to dispense the dose of medicine through the infusion tubing **147** into the infusion set **146** and cannula **149**. After the pump drive cycle **1632** is activated, the control circuitry may then standby **1634** prior to the next pump drive cycle (e.g., in accordance with a previously determined basal dosage schedule or a requested bolus dosage) before executing process **1600** again.

A number of embodiments of the invention have been described. Nevertheless, it will be understood that various modifications may be made without departing from the spirit and scope of the invention. Accordingly, other embodiments are within the scope of the following claims.

What is claimed is:

1. An occlusion sensor system for detecting an occlusion in a flow path from an insulin infusion pump system, the occlusion sensor system comprising:

a fluid channel that at least partially defines an insulin flow path between an insulin reservoir and an output port;

a flexible membrane in fluid communication with the fluid channel so that fluid pressure in the fluid channel acts upon the flexible membrane;

an air cavity positioned adjacent to the flexible membrane and generally opposite the fluid channel;

a light transmissive member adjacent to the air cavity, the light transmissive member being arranged opposite the flexible membrane such that fluid pressure in the fluid

channel above a threshold value causes the flexible membrane to deform into the air cavity and toward the light transmissive member;

a primary light emitter configured to align with the light transmissive member and emit light into the light transmissive member;

a light sensor configured to align with the light transmissive member and receive light from the primary light emitter that passes through the light transmissive member; and

a reference light emitter configured to emit light that is received by the light sensor, wherein the reference light emitter is spaced apart from the primary light emitter.

2. The occlusion sensor system of claim **1**, wherein the reference light emitter is spaced apart from the primary light emitter such that the light emitted from the reference light emitter is received by the light sensor without passing through the light transmissive member.

3. The occlusion sensor system of claim **1**, further comprising control circuitry electrically connected to the primary light emitter, the reference light emitter, and the light sensor, wherein the control circuitry activates the primary light emitter in isolation from activation of the reference light emitter.

4. The occlusion sensor system of claim **3**, wherein the control circuitry compares a first value indicative of light detected at the light sensor from the primary light emitter to a second value indicative of light detected at the light sensor from the reference light emitter.

5. The occlusion sensor system of claim **4**, wherein in response to the comparison of the first value to the second value being outside of a threshold range, the control circuitry generates an occlusion alarm output from the infusion pump system.

6. The occlusion sensor system of claim **1**, wherein the light sensor receives light from the primary light emitter that is internally reflected by the light transmissive member, the light transmissive member having two generally flat surfaces through which the light from the primary light emitter enters and exits the light transmissive member.

7. The occlusion sensor system of claim **1**, wherein when the flexible membrane is in a non-abutting position with the light transmissive member, the light from the light emitter undergoes total internal reflection within the light transmissive member at an interface with the air cavity.

8. The occlusion sensor system of claim **7**, wherein in response to an occlusion in a flow path extending from the fluid channel, the flexible membrane is adjustable to abut the light transmissive member.

9. The occlusion sensor system of claim **8**, wherein when the flexible membrane abuts the light transmissive member, at least a portion the light from the primary light emitter passes from the light transmissive member and into the flexible membrane at an interface between the light transmissive member and the flexible membrane.

10. The occlusion sensor system of claim **1**, wherein the light sensor, the primary light emitter, and the reference light emitter are housed in a reusable controller device while the flexible membrane, the air cavity, and the light transmissive member are components of a cap device that attaches to a disposable pump device configured to removably attach to the reusable controller device.

11. An occlusion sensor system for an infusion pump system including a reusable controller device that is removably attachable to a disposable single-use pump device that defines a space to receive medicine therein, the occlusion sensor system comprising:

a primary light emitter, a reference light emitter, and a light sensor arranged in the reusable controller device, wherein the primary light emitter, the reference light emitter, and the light sensor are in electrical communication with control circuitry housed inside the reusable controller device; and

a light transmissive member arranged in the disposable single-use pump device, the light transmissive member being aligned with the primary light emitter and the light sensor when the reusable controller device is removably attached to a disposable single-use pump device;

wherein in response to activation of the primary light emitter, the light sensor receives at least a portion of the light from the primary light emitter that passes through the light transmissive member, and

wherein in response to activation of the reference light emitter, the light sensor receives a least a portion of the light that is emitted from the reference light emitter without passing through the light transmissive member.

12. The occlusion sensor system of claim **11**, further comprising: a cavity positioned adjacent to the light transmissive member, a flexible membrane that defines at least one wall of the air cavity and that is arranged in the disposable single-use pump device, and a fluid channel that at least partially defines a medicine flow path between the medicine reservoir reservoir and an output port, the fluid channel being in fluid communication with the flexible membrane so that fluid pressure in the fluid channel acts upon the flexible membrane.

13. The occlusion sensor system of claim **12**, wherein when the flexible membrane is in a first operative position, the light from the primary light emitter undergoes total internal reflection within the light transmissive member at an interface with the cavity.

14. The occlusion sensor system of claim **13**, wherein in response to a flow condition in a flow path extending from the disposable single-use pump device, the flexible membrane is adjustable to a second operative position in which the flexible membrane abuts the light transmissive member.

15. The occlusion sensor system of claim **11**, further comprising control circuitry housed in the reusable controller device and electrically connected to the primary light emitter, the reference light emitter, and the light sensor, wherein the control circuitry activates the primary light emitter at a time different from activation of the reference light emitter.

16. The occlusion sensor system of claim **15**, wherein the control circuitry compares a first value indicative of light detected at the light sensor from the primary light emitter to a second value indicative of light detected at the light sensor from the reference light emitter.

17. The occlusion sensor system of claim **16**, wherein in response to the comparison of the first value to the second value being outside of a threshold range, the control circuitry generates an occlusion alarm output from the infusion pump system.

18. An occlusion sensor system for detecting an occlusion in a flow path from an insulin infusion pump system, the occlusion sensor system comprising:

a primary light emitter configured to emit light toward an insulin flow path;

a light sensor configured to receive at least a portion of the light from the primary light emitter after the light is emitted toward the insulin flow path, wherein the light sensor outputs an electrical signal in response to receiving light;

a reference light emitter configured to emit light that is received by the light sensor, wherein the reference light emitter is separate from the primary light emitter; and

control circuitry electrically connected to the primary light emitter, the reference light emitter, and the light sensor, wherein the control circuitry compares a first value indicative of light detected at the light sensor from the primary light emitter to a second value indicative of light detected at the light sensor from the reference light emitter, and in response to the comparison of the first value to the second value being outside of a threshold range, the control circuitry generates an occlusion alarm for output via a user interface.

19. The occlusion sensor system of claim **18**, further comprising: a flexible membrane in fluid communication with the insulin flow path so that fluid pressure from the insulin flow path acts upon the flexible membrane; a cavity positioned adjacent to the flexible membrane and generally opposite the insulin flow path; and a light transmissive member adjacent to the cavity, the light transmissive member being arranged opposite the flexible membrane such that fluid pressure in the insulin flow path above a threshold value causes the flexible membrane to deform into the cavity and toward the light transmissive member, wherein the primary light emitter is configured to align with the light transmissive member and emit light into the light transmissive member.

20. The occlusion sensor system of claim **19**, wherein the light sensor, the primary light emitter, and the reference light emitter are housed in a reusable controller device while the flexible membrane, the cavity, and the light transmissive member are components of a cap device that attaches to a disposable pump device configured to removably attach to the reusable controller device.

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