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**Lee**

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(54) **AUTOMATED PLANNING VOLUME  
CONTOURING ALGORITHM FOR  
ADJUVANT BRACHYTHERAPY  
TREATMENT PLANNING IN SARCOMA**

(75) Inventor: **Eva K. Lee**, Atlanta, GA (US)

(73) Assignee: **Georgia Tech Research Corporation**,  
Atlanta, GA (US)

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**G01B 13/20** (2006.01)

(52) **U.S. Cl.** ..... **600/424; 702/19; 702/156**

(58) **Field of Classification Search** ..... **702/19,**  
**702/156; 600/424**

See application file for complete search history.

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*Primary Examiner*—Michael Borin

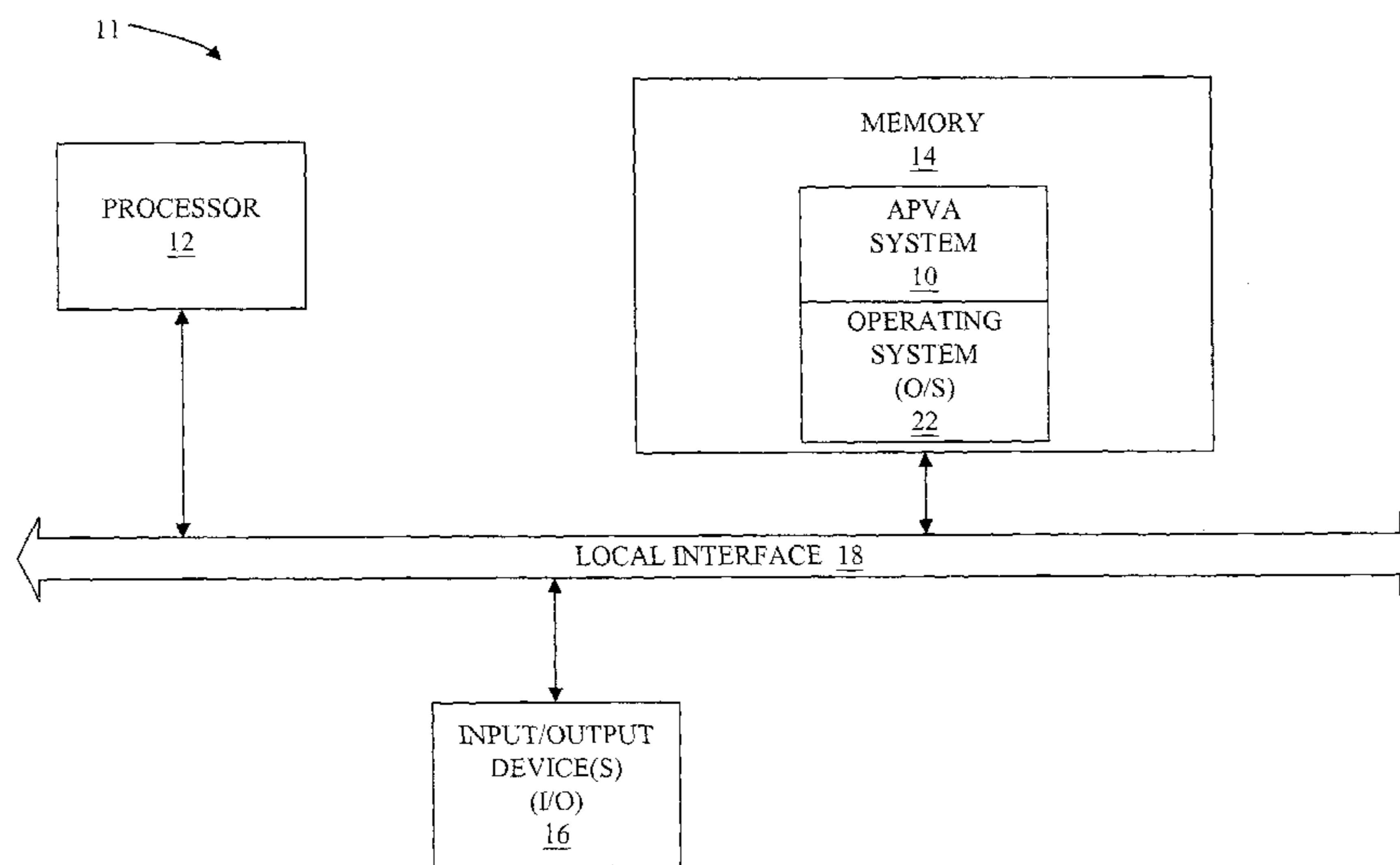
(74) *Attorney, Agent, or Firm*—Thomas, Kayden,  
Horstemeyer & Risley, LLP

(57)

**ABSTRACT**

A mathematical contouring algorithm that automatically  
determines the planning volume of a sarcoma prior to  
designing a brachytherapy treatment plan. The algorithm,  
utilizing computational geometry, numerical interpolation  
and artificial intelligence (AI) techniques, returns the plan-  
ning volume in digitized and graphical forms in a matter of  
minutes. Such an automatic procedure reduces labor time  
and provides a consistent and objective method for deter-  
mining planning volumes. In addition, a definitive represen-  
tation of the planning volume allows for sophisticated  
brachytherapy treatment planning approaches to be applied  
when designing treatment plans, so as to maximize local  
tumor control and minimize normal tissue complications.

**22 Claims, 13 Drawing Sheets**



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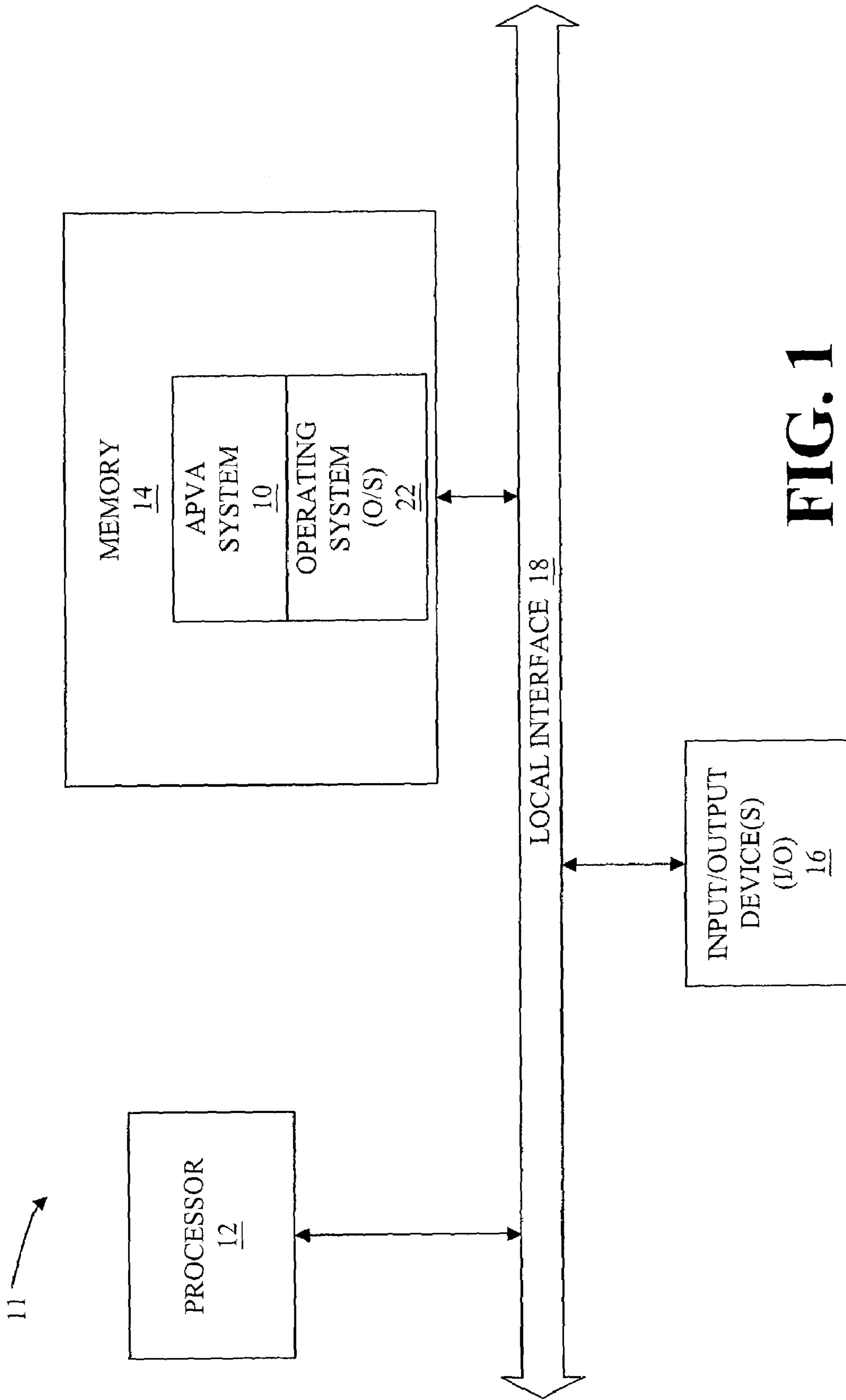
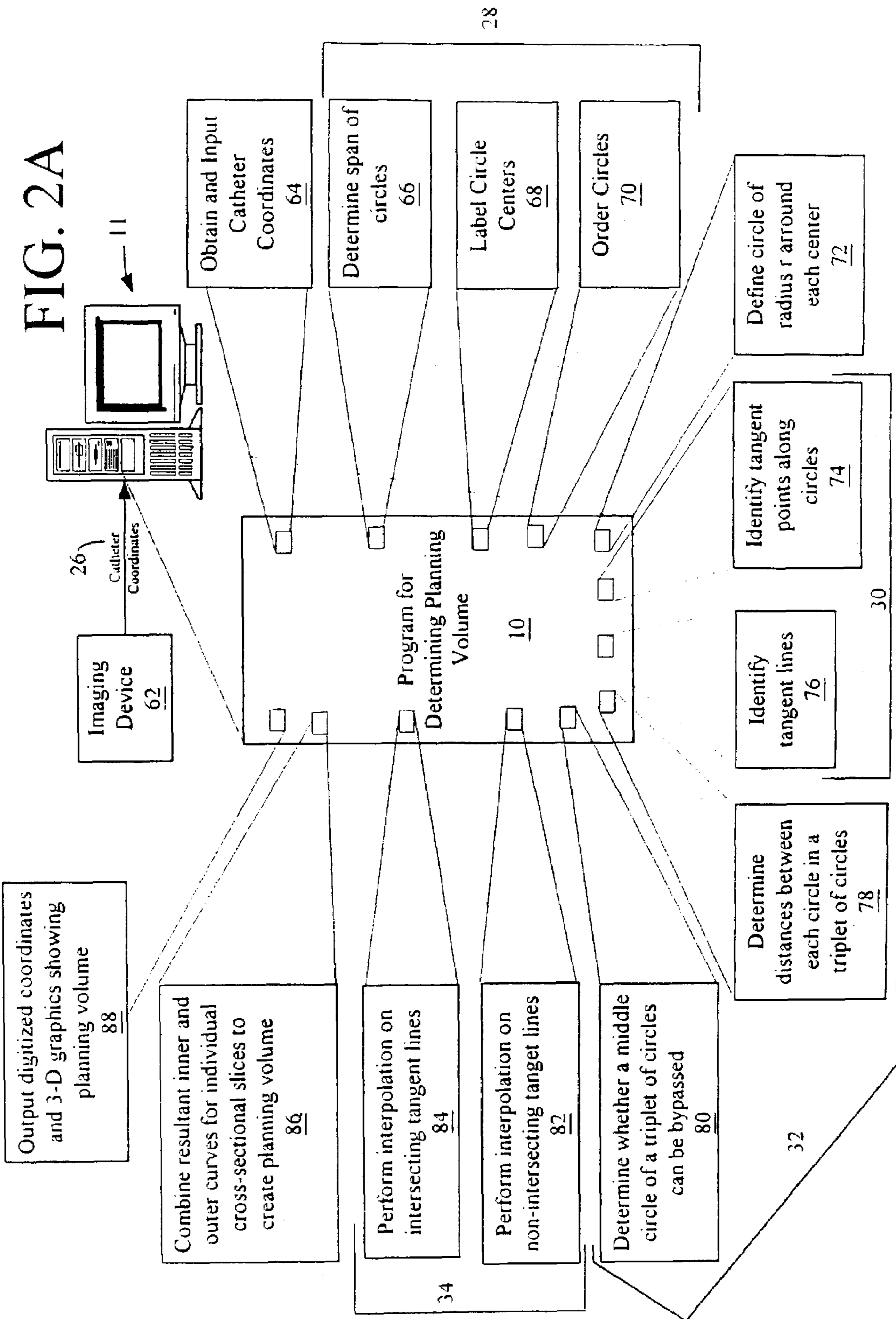
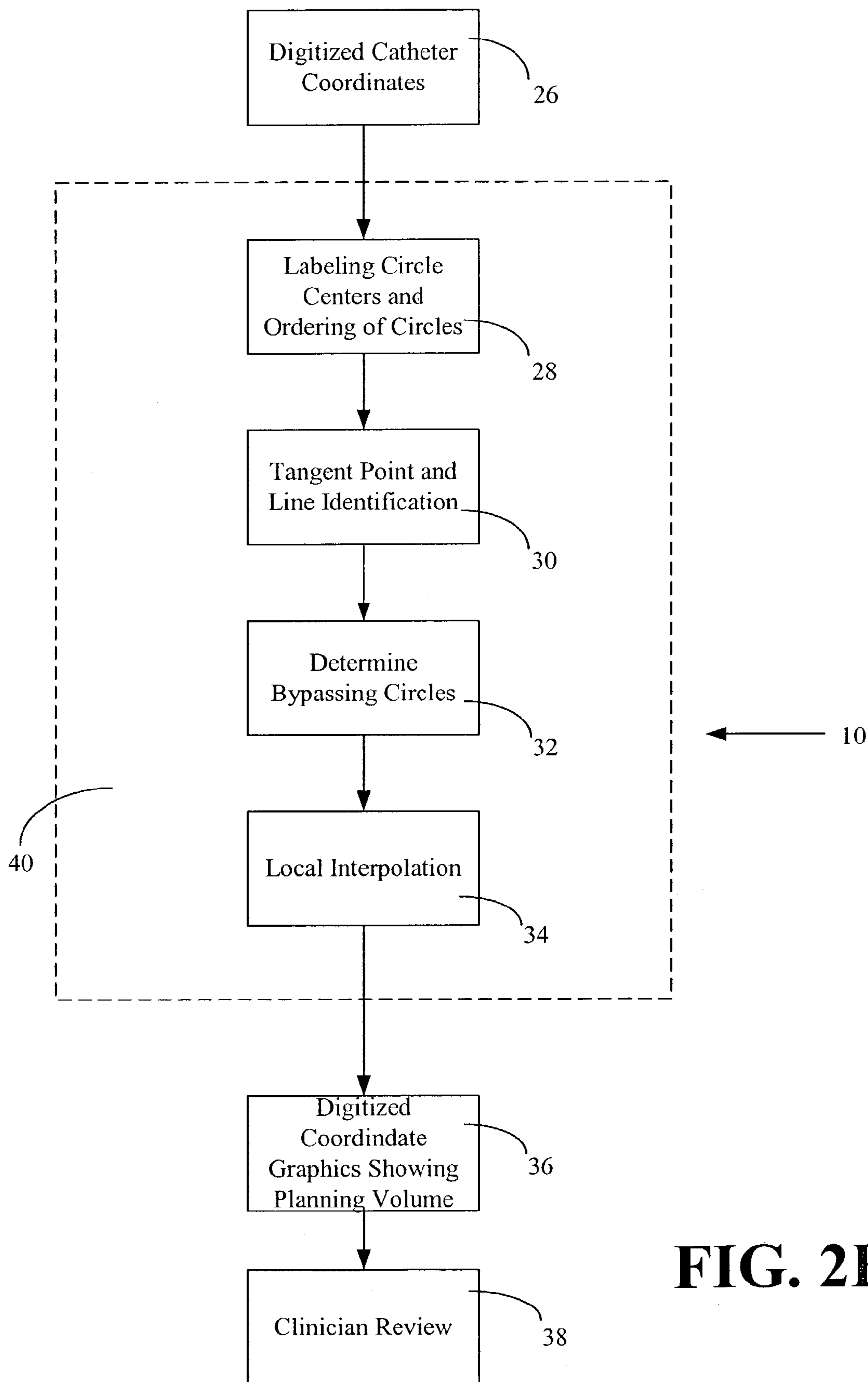


FIG. 1





**FIG. 2B**

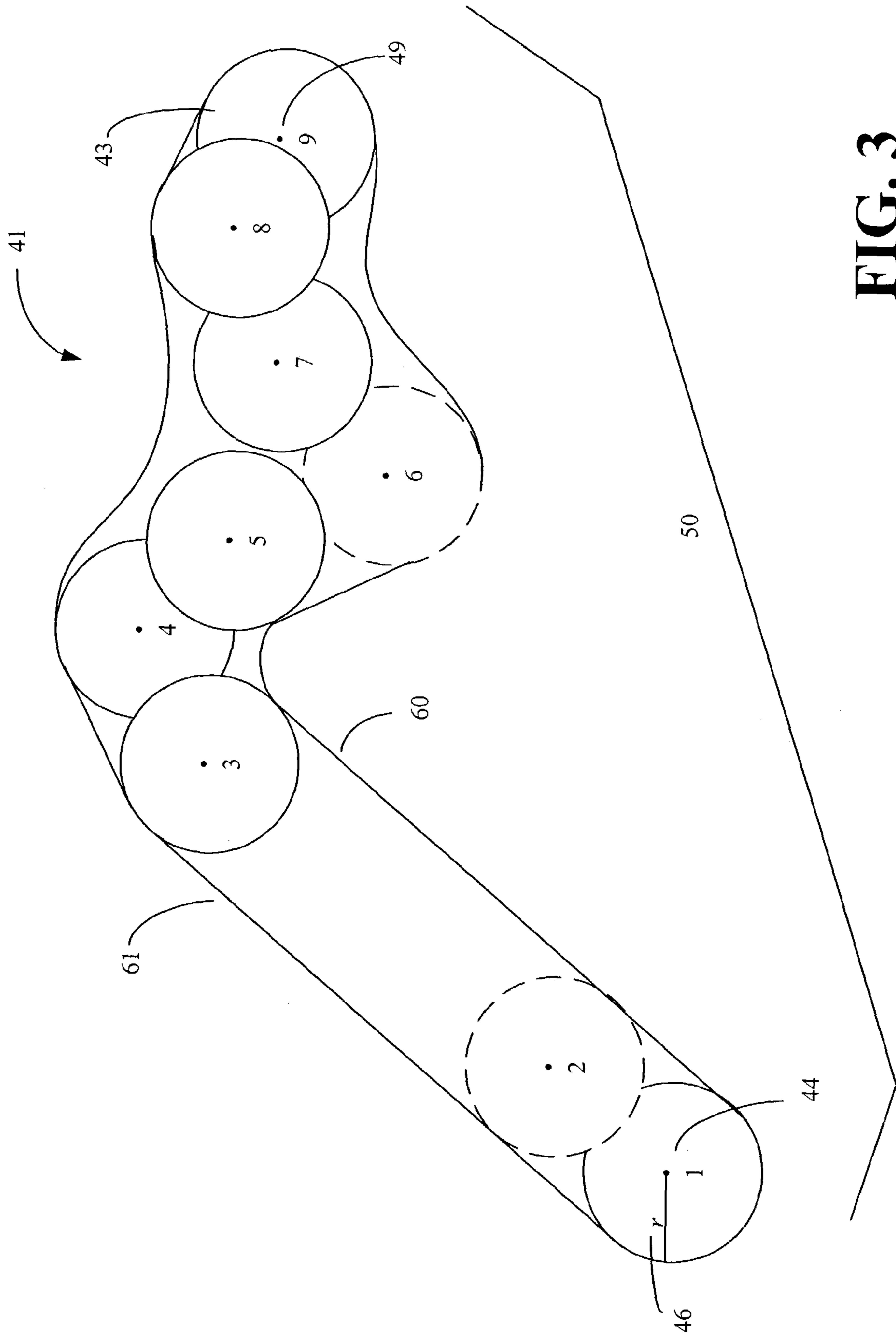
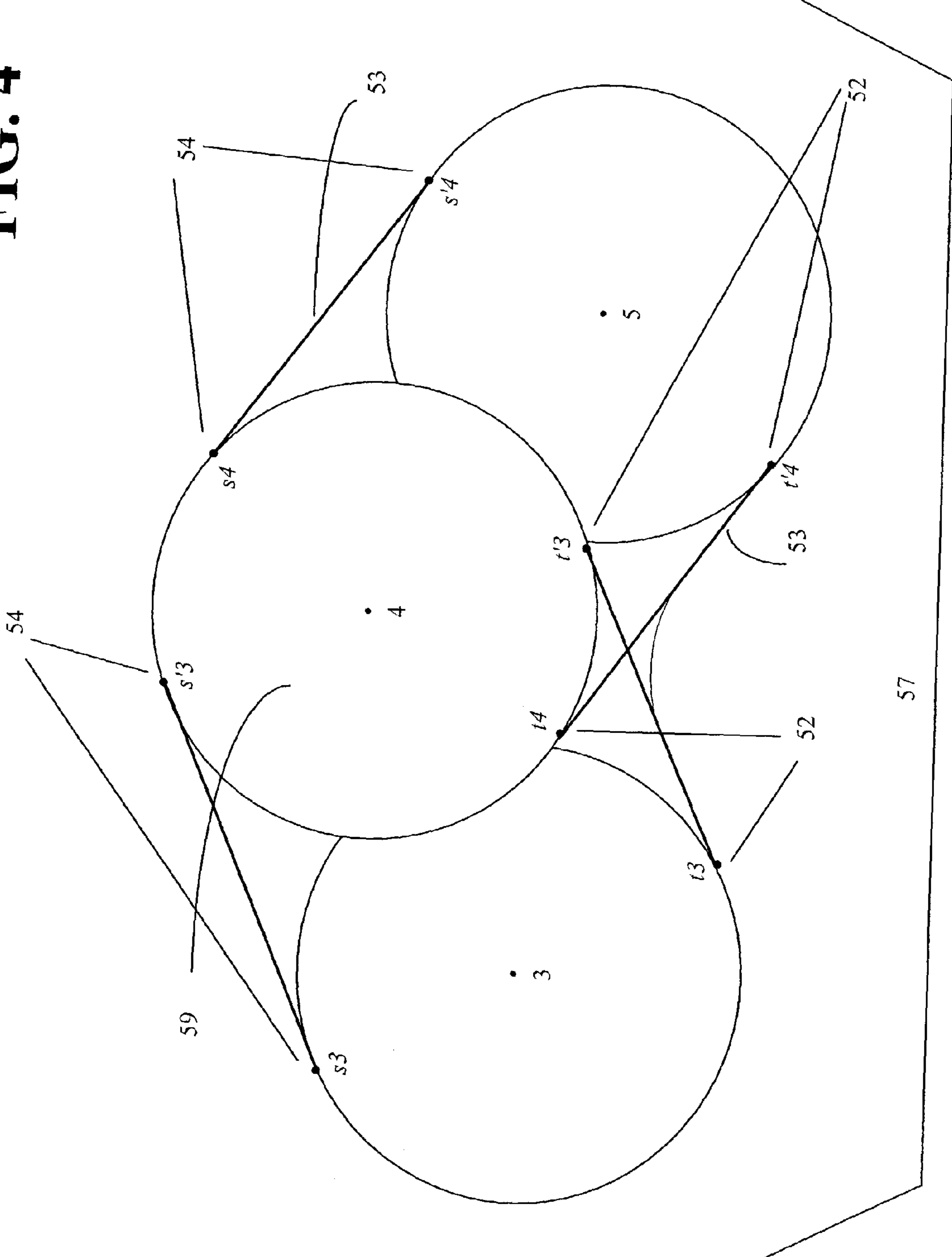


FIG. 3

FIG. 4



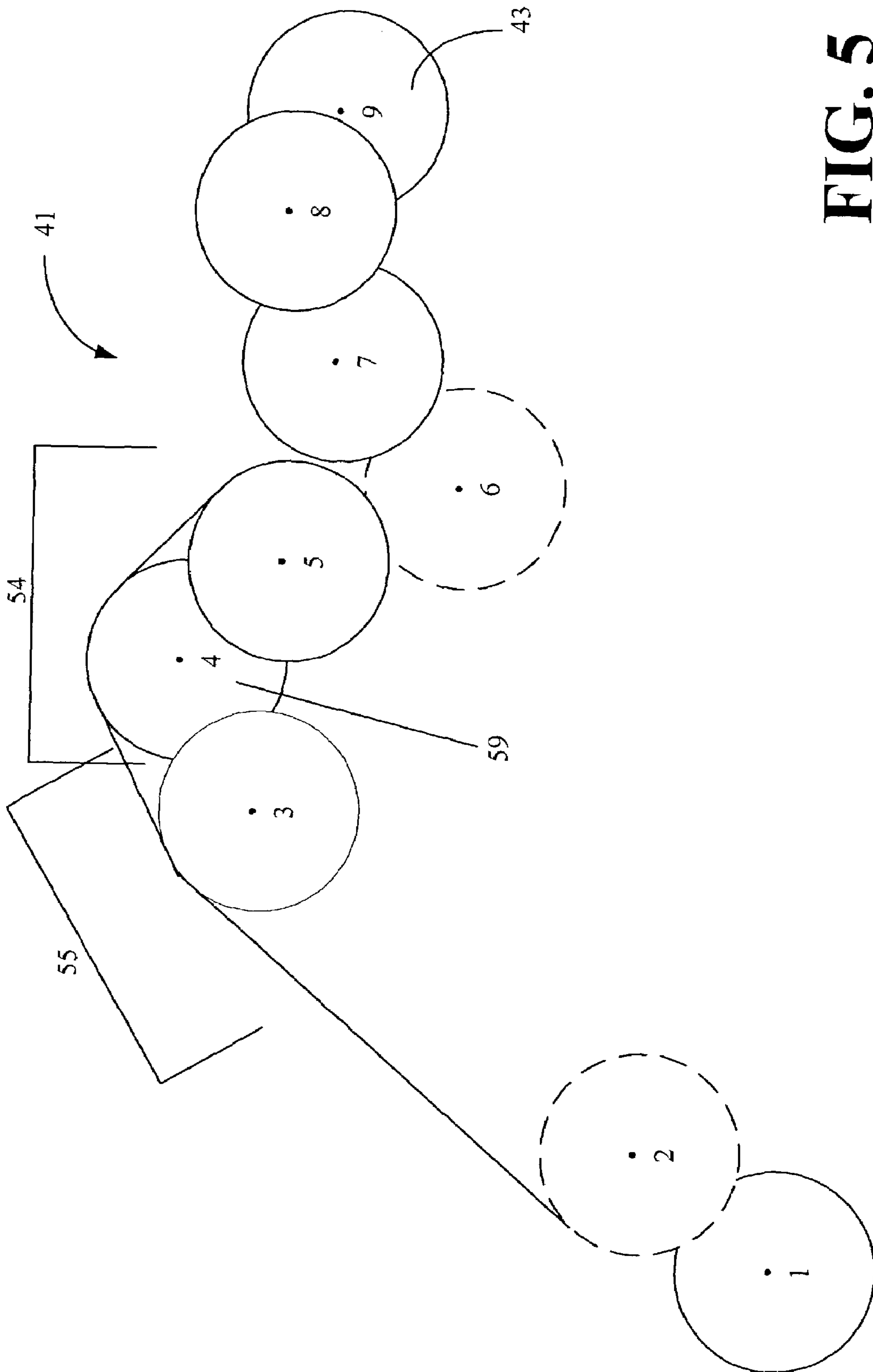


FIG. 5



FIG. 6

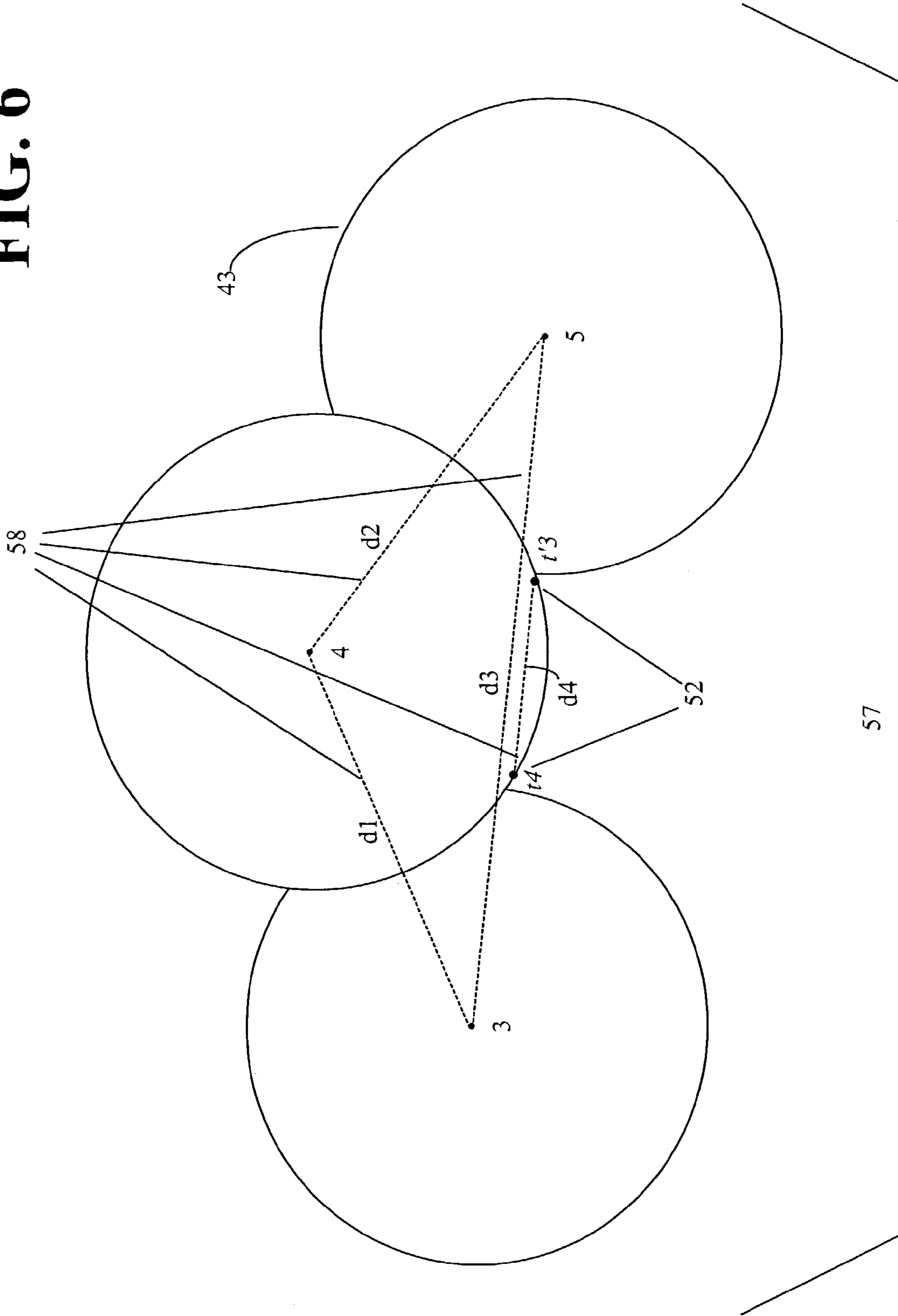


FIG. 7A

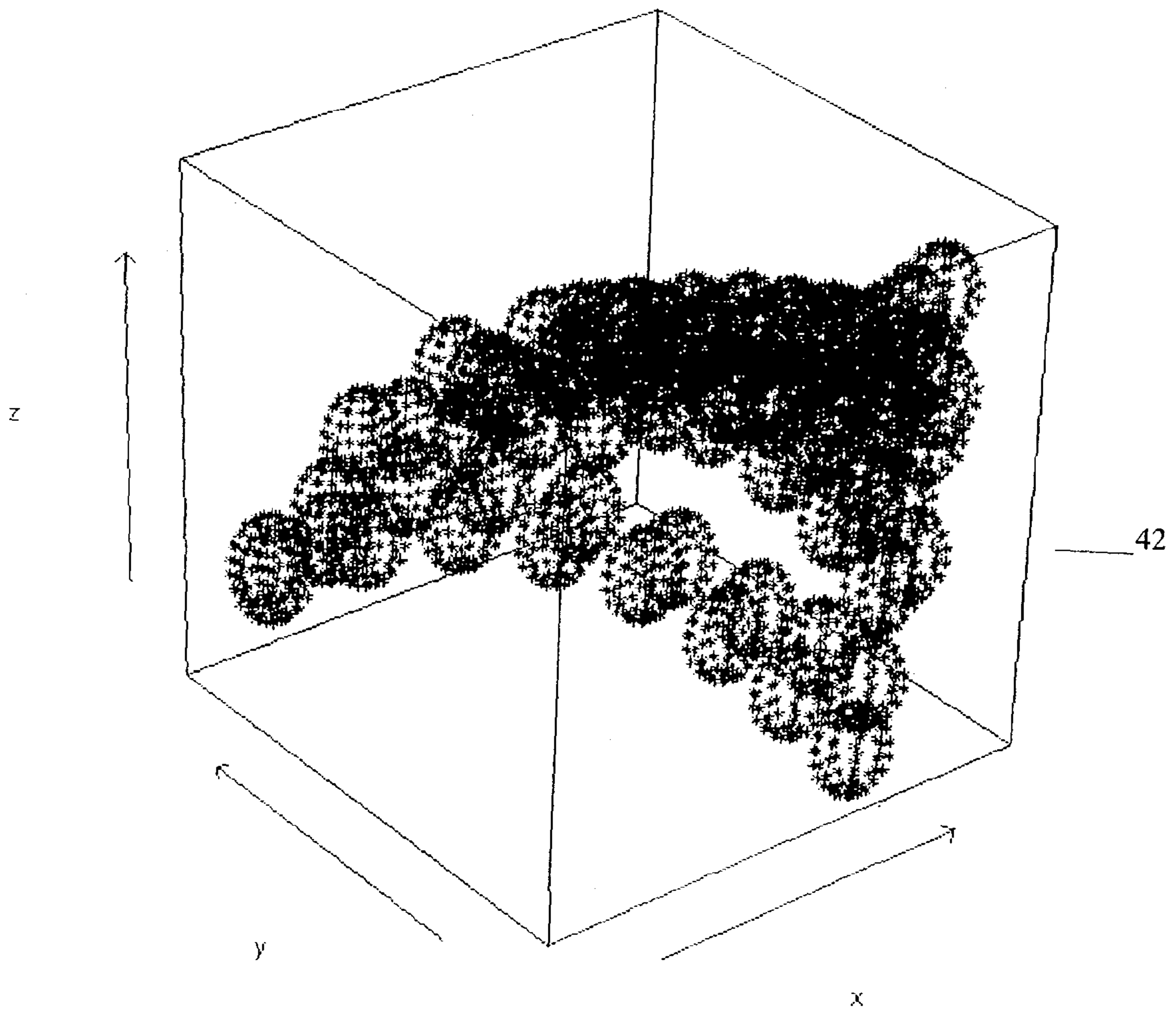


FIG. 7B

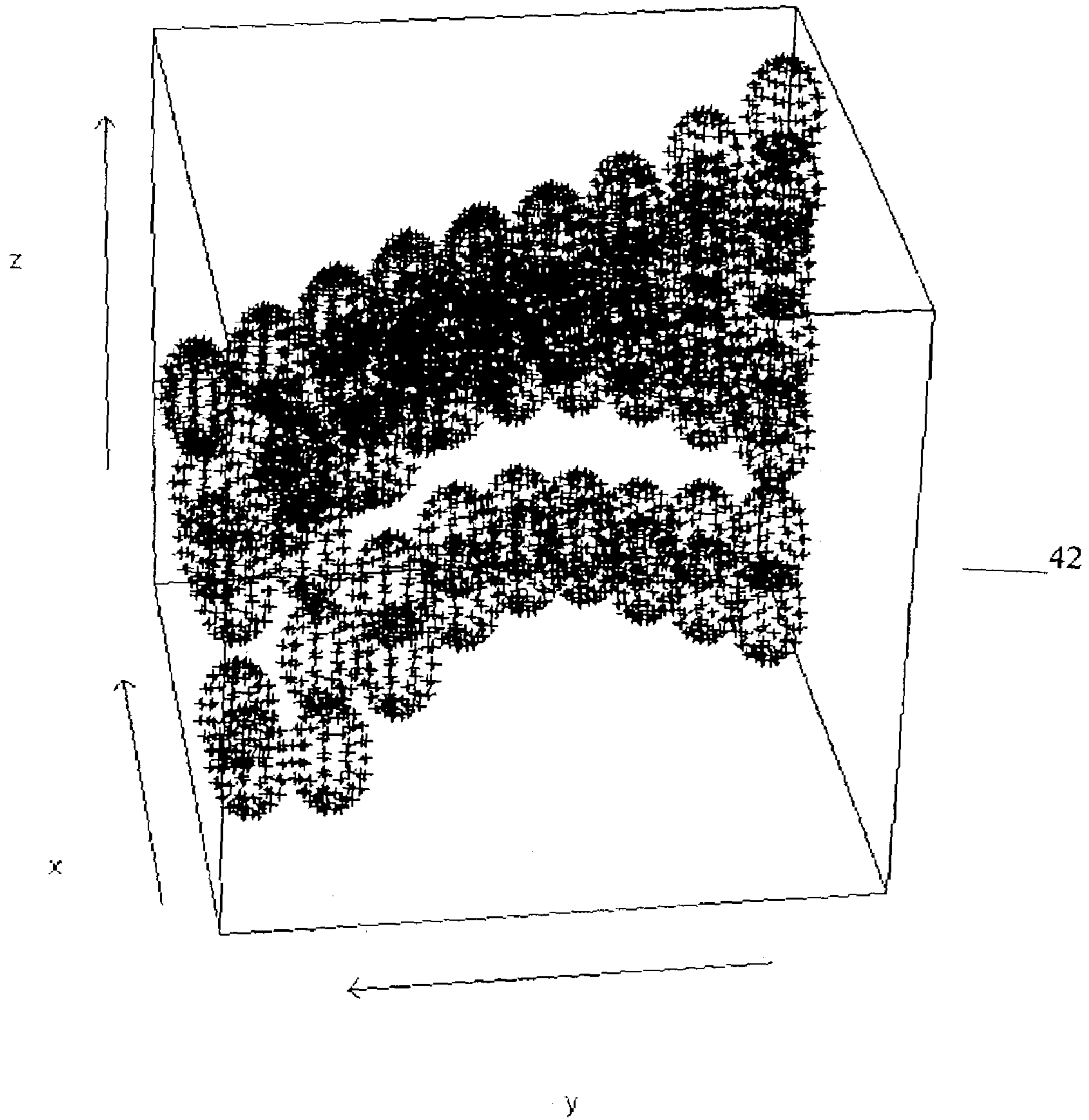


FIG. 7C

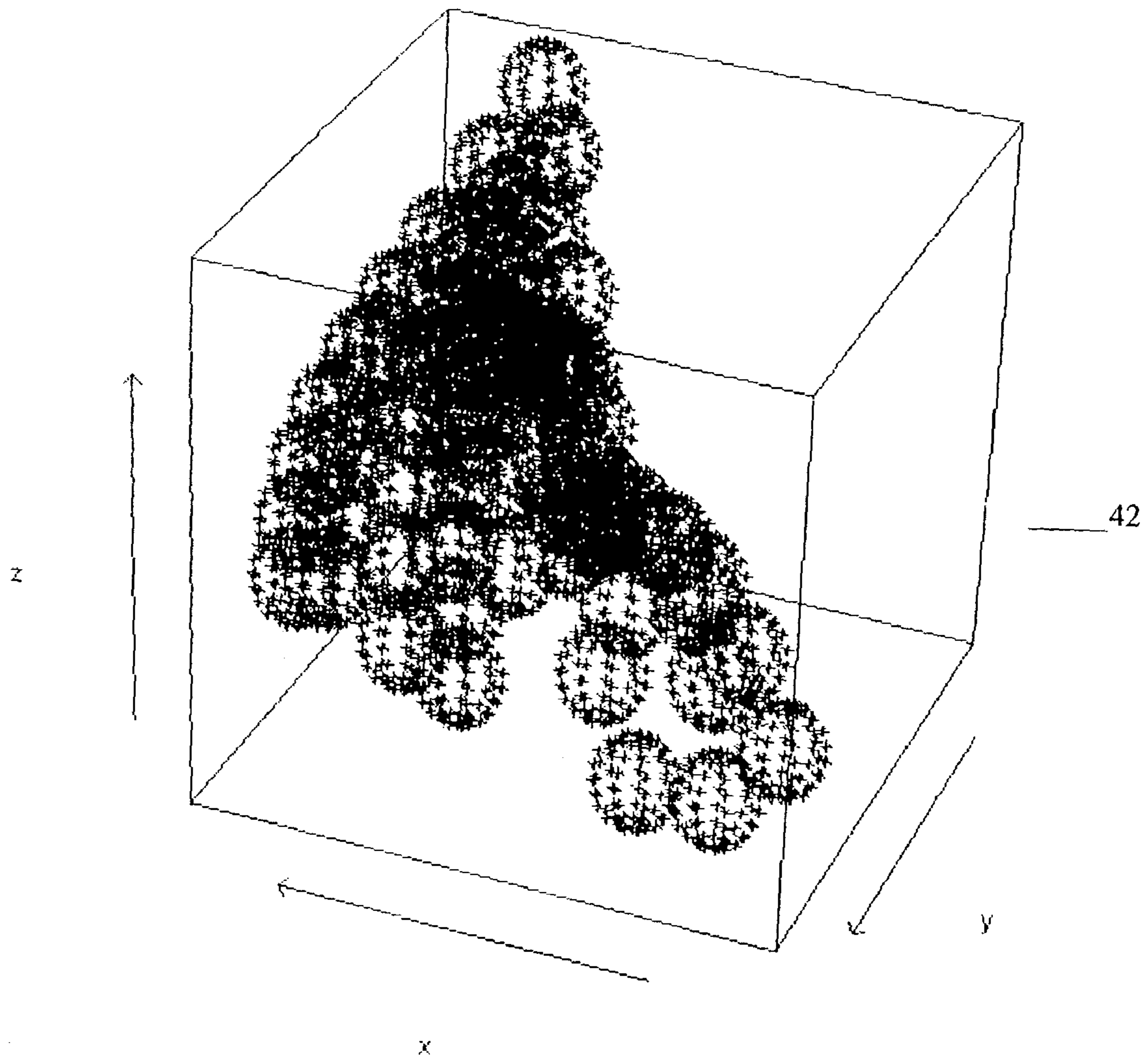


FIG. 7D

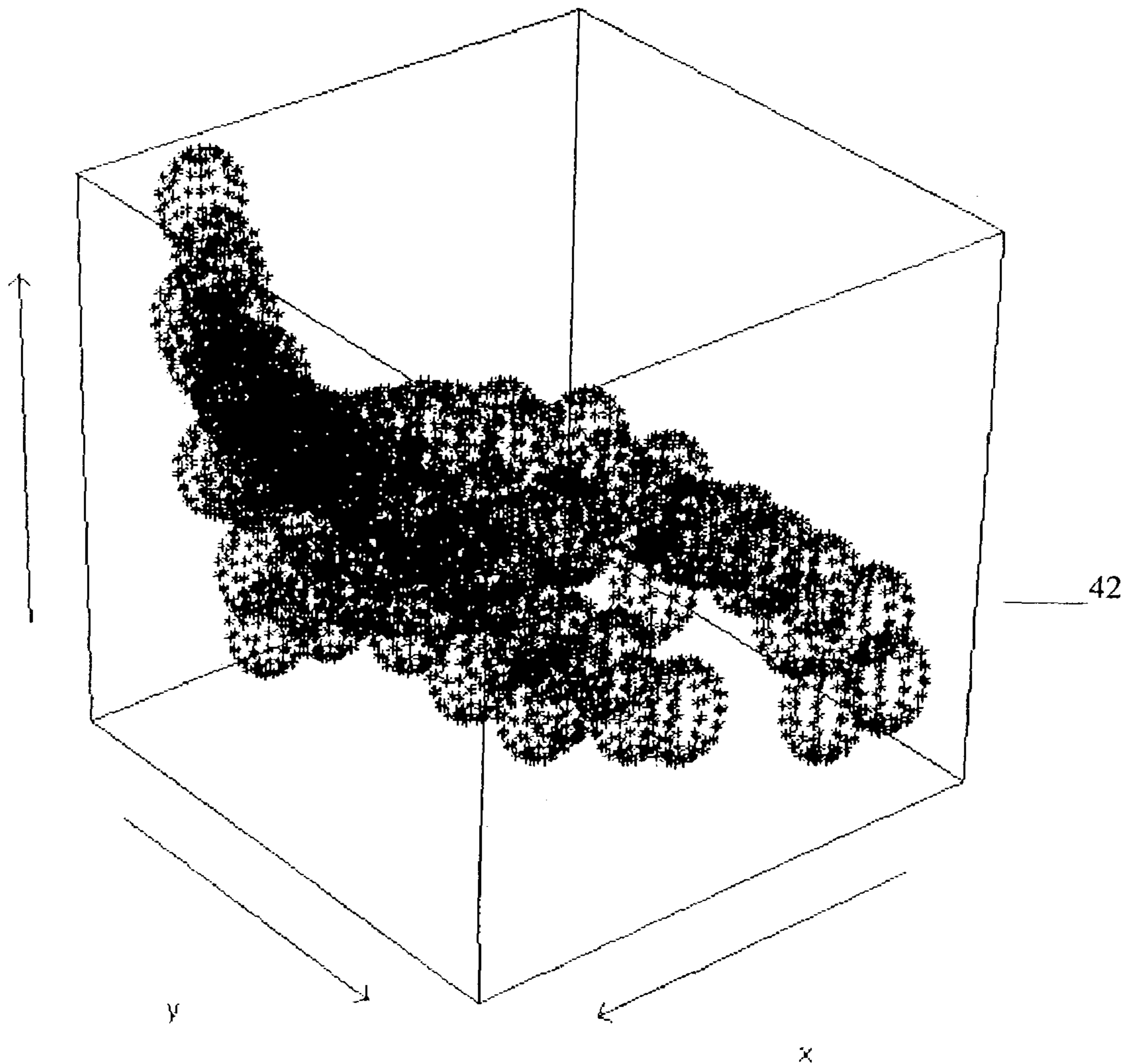


FIG. 7E

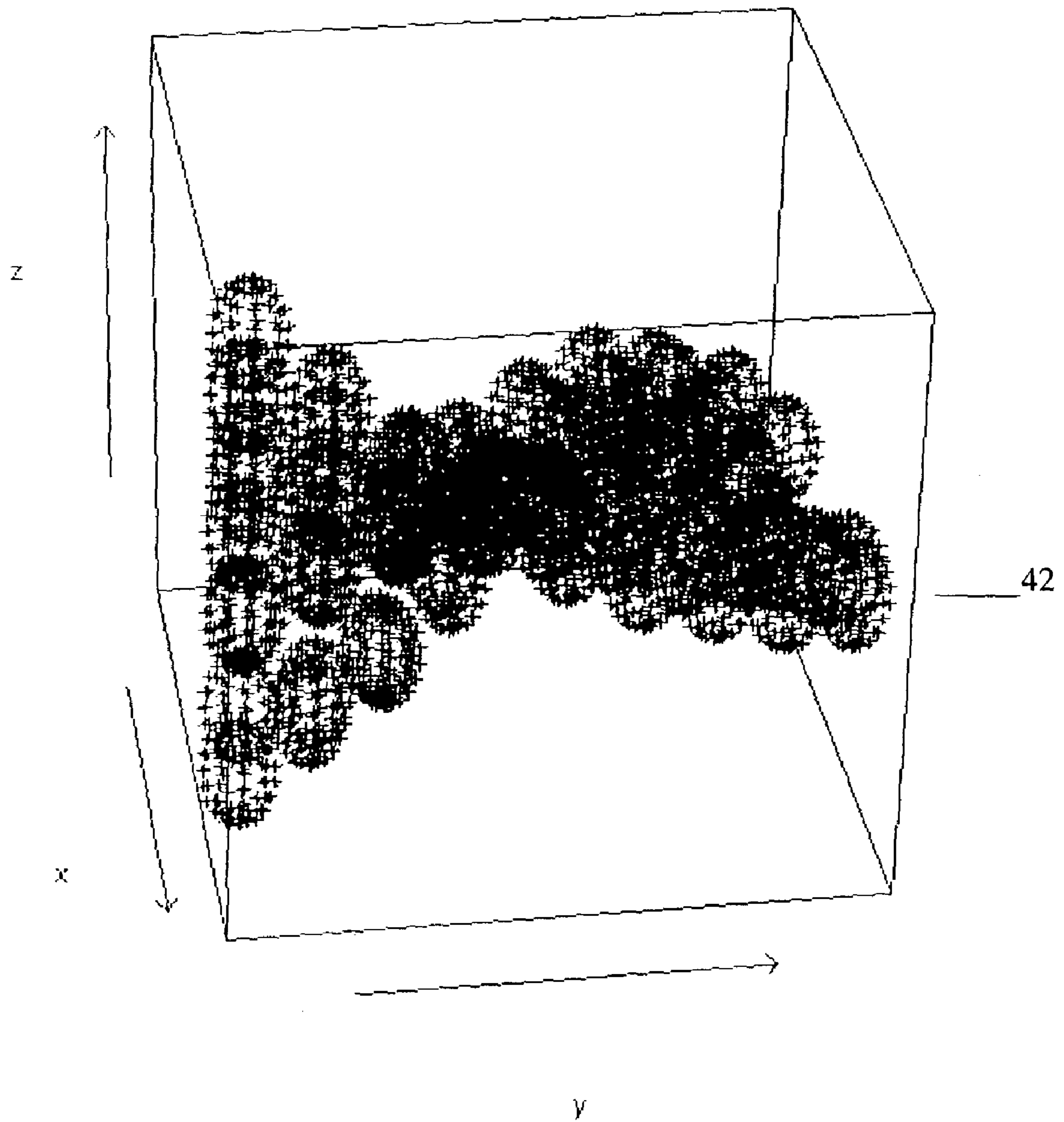
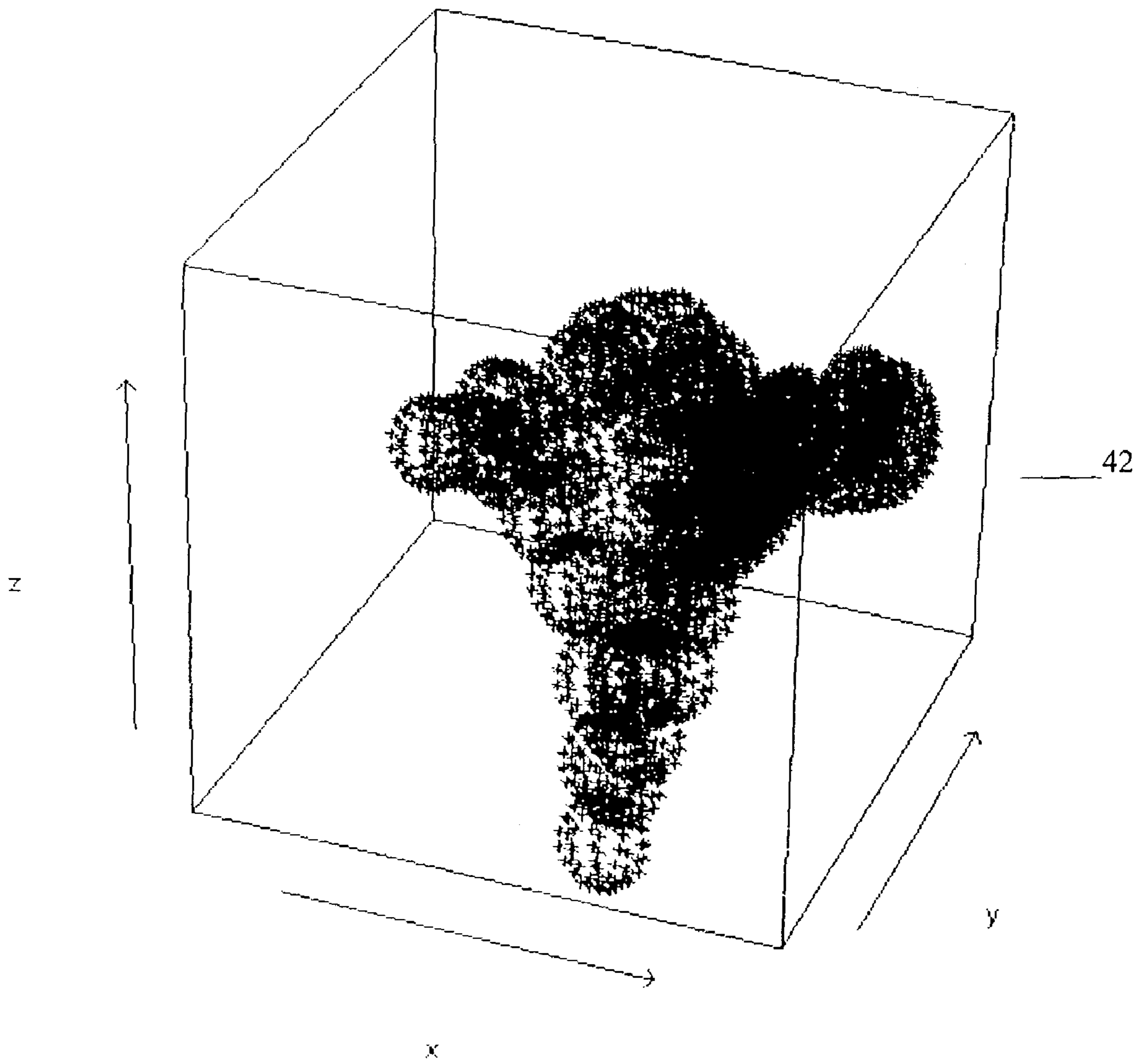


FIG. 7F



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**AUTOMATED PLANNING VOLUME  
CONTOURING ALGORITHM FOR  
ADJUVANT BRACHYTHERAPY  
TREATMENT PLANNING IN SARCOMA**

CROSS-REFERENCE TO RELATED  
APPLICATION

This application is a divisional of copending U.S. utility application entitled, "Automated Planning Volume Contouring Algorithm for Adjuvant Brachytherapy Treatment Planning in Sarcoma," having Ser. No. 09/872,118, filed Jun. 1, 2001, now U.S. Pat. No. 6,615,070, which is entirely incorporated herein by reference which claims the benefit of Provisional application Ser. No. 60/208,608, filed Jun. 1, 2000.

TECHNICAL FIELD

The present invention is generally related to using computational geometry and numerical interpolation techniques to develop a procedure that automatically outlines the contours of the planning volume for sarcoma tumor beds prior to designing brachytherapy treatment plans for soft-tissue sarcoma.

BACKGROUND OF THE INVENTION

Soft-tissue sarcomas are tumors that arise in the soft tissues that connect, support and surround other parts of the body, such as muscles, tendons, fat, joint linings, and blood vessels. Although about one-half of the cases occur in the arms and legs, soft-tissue sarcomas are known to develop at any site in the body. Sarcoma tumors occur primarily in the second and sixth decades of life, but may occur at any age and, typically, the incidence rises with increasing age and is more prevalent in men.

There are more than fifty different types of soft-tissue sarcomas and sarcoma-like growths, at least thirty-five of which are malignant. Approximately 6,000 new cases of soft-tissue sarcoma are diagnosed each year in the United States. Additionally, the large majority of soft-tissue sarcomas are greater than 5 cm in size, requiring a combination of treatment techniques. Fortunately, soft-tissue sarcomas are relatively rare, representing only about one percent of all cancer cases, but they provide unique challenges in detection and treatment.

In the past, the standard treatment for soft-tissue sarcoma included amputation of limbs or radical surgery. In current practice, soft-tissue sarcomas are typically treated with a more conservative surgery combined with radiation therapy. The surgical removal of the tumor is the primary treatment. However, adjuvant (or additional) treatment with radiation therapy greatly increases the effectiveness of sarcoma treatment. Radiation therapy may be used before, during and/or after the surgical removal of the sarcoma. Typically, treatment involving both surgery and radiation therapy will include external-beam radiotherapy or brachytherapy.

Brachytherapy is an advanced cancer treatment that delivers radiation therapy from within the body (as opposed to external application of radiation to the tumor and surrounding tissues). The benefit of brachytherapy is that a high dose of radiation may be applied to the tumor or tumor bed (where the tumor was removed) while reducing the dose to surrounding healthy tissues.

In application, brachytherapy may be used to treat soft-tissue sarcomas in two ways. In one approach, during

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surgery, after the surgeon removes the tumor, the radiation oncologist implants a series of catheters into the tumor bed. Several days after the operation, radiotherapeutic seeds are inserted into each of these catheter tubes. These seeds stay in the catheter tubes for several days, delivering a high dose of radiotherapy to the area of the tumor. When the treatment is completed, both the radiotherapeutic seeds and the catheters are removed. The second form of brachytherapy is called high dose rate intra-operative radiation therapy. In this procedure, all the radiotherapy is actually delivered during the operation. This procedure requires a specially shielded operating room where both the surgery and the radiation therapy can be given. However, the high dose rate approach often requires a subsequent course of external beam radiation therapy.

The form of adjuvant brachytherapy in which catheters filled with radioactive seeds are inserted into the tumor or tumor bed is promising. However, this technique is limited by the difficulties of precisely placing catheter tubes into position and applying the correct amount of radiation to the affected areas while limiting the exposure of "healthy" tissues to the radiation. Several factors contribute to the difficulty of applying this treatment modality to soft-tissue sarcoma. First, each anatomical site and associated patient/tumor geometry is unique. Second, the tumor bed is usually of irregular shape. Third, the catheters, inserted during surgery, are often non-uniformly spaced and non-coplanar. Any of these factors may result in over or under treating the affected areas, as well as radiating healthy tissues.

In current practice, the planning volume for adjuvant brachytherapy treatment for soft-tissue sarcoma is typically derived via a tedious manual process, often resulting in the volume of the sarcoma not being appropriately determined. In the manual process, the outline of the volume is determined based on the positions of the catheters by hand calculations and planner observations. The current process for determining the planning volume is subjective, inconsistent, time-consuming, and highly dependent on the human planner. Thus, the current methods for determining the planning volume of sarcomas for brachytherapy may result in variability in the placement of the radiation seeds inside the catheters and variability in the distribution of radiation to the sarcoma bed.

In order to provide the most effective radiation therapy, the radiation dose distribution must cover all of the tumor bed and at the same time affect as little as possible of the healthy surrounding tissue. The ultimate location of the radiation seeds is one of the most important factors affecting the radiation dose distribution. Since the desired dose distribution is affected by the planning volume and the placement of the catheters and radiation seeds, the accurate derivation of the planning volume is a fundamental problem. The current practice does not provide a consistent, efficient and accurate method for determining the planning volume.

Thus, a heretofore unaddressed need exists in the industry to address the aforementioned deficiencies and inadequacies.

SUMMARY OF THE INVENTION

In order to increase the effectiveness of catheter brachytherapy treatment, the delivery of the radioactive sources to the affected areas (or planning volume) is critical. The present invention focuses on the automated generation of planning tumor volumes for the treatment of soft-tissue sarcomas. By using an automated contouring algorithm the planning tumor volume can be determined and the optimal



placement and insertion of radioactive seeds can be designed to provide the most effective brachytherapy treatment.

The present invention provides a system and method for automatically determining the planning volume of a sarcoma by algorithmic manipulation of catheter coordinate input data. Initially, the catheters are inserted into the sarcoma bed during a surgical procedure. The volume of the sarcoma is divided into cross-sectional slices in which the catheters appear as "centers." Around these centers, a circle having a certain radius is drawn. The radius of the circles is an indicator of the area over which the radioactive seeds will provide effective treatment. By configuring the radii of the circles to have sufficient size, the entire surface of each of the cross-sectional slices may be covered and, therefore, treated with the radioactive seeds. Optimally, the circles are configured such that all areas of the sarcoma receive treatment, while only a minimum of healthy tissue is exposed to the radiation.

The automated planning volume algorithm is comprised of a number of subroutines or sub-algorithms. The algorithm, utilizing computational geometry, numerical interpolation, and artificial intelligence (AI) techniques to manipulate the catheter coordinates, returns the planning volume in digitized and graphical forms in a matter of minutes. After the coordinates are inputted, the algorithm will automatically determine the "span," or furthest distance between centers, and order the circles in a normal numerical progression. The algorithm is able to self-correct the numbering of the centers such that a smooth curve is defined which encompasses the affected tissue and limits incorporation of healthy tissue within the curves. Then, the algorithm selects tangent points for each circle and determines the corresponding tangent lines for groups of circles. By iteration of the tangent lines, the algorithm generates a series of curves. These curves provide the overall shape of the surface of each cross-sectional slice. The shapes of the individual slices may then be compiled so as to provide the overall shape and volume of the sarcoma bed. The algorithm outputs the resultant volume data as a graphical representation of the planning volume and the location of the digitized catheter coordinates therein.

The automatic generation of sarcoma planning volumes is a fast and efficient way to consistently and accurately determine planning volumes. Instead, of performing lengthy and difficult calculations by hand, the clinician may simply input the catheter coordinates for each slice, wait a few minutes for the algorithm to compute the data and generate the graphical outputs, and then review and evaluate the outputs. The automated approach provides a definitive representation of the planning volume and will allow for the application of more sophisticated brachytherapy treatment planning designs. Ultimately, the detailed volume graphics and coordinate data will aid in developing treatment plans that maximize local tumor control and minimize normal tissue complications.

Other systems, methods, features, and advantages of the present invention will be or become apparent to one with skill in the art upon examination of the following drawings and detailed description. It is intended that all such additional systems, methods, features, and advantages be included within this description, be within the scope of the present invention, and be protected by the accompanying claims.

#### BRIEF DESCRIPTION OF THE DRAWINGS

The invention can be better understood with reference to the following drawings. The components in the drawings are not necessarily to scale, emphasis instead being placed upon clearly illustrating the principles of the present invention. Moreover, in the drawings, like reference numerals designate corresponding parts throughout the several views.

FIG. 1 is a block diagram showing the implementation of the automated planning volume system.

FIG. 2A is a block diagram illustrating an imaging device and its input into a computer, and further illustrating the automated planning volume system and the steps executed thereby to generate the planning volume.

FIG. 2B is a block diagram showing the algorithmic steps of the automated planning volume system of FIG. 1.

FIG. 3 is a graphical representation of a cross-sectional slice showing nine catheter insertions, circles of radii  $r$  around the catheter centers, and the natural ordering of the circle centers from the origin to the destination.

FIG. 4 is a graphical representation of circles 3, 4 and 5 of FIG. 3, illustrating the construction of the tangent points and the corresponding interpolation of the inner curve.

FIG. 5 is a graphical representation focussing on circles 3, 4, 5 and 6 of FIG. 3, illustrating the construction of part of the curve for the planning volume.

FIG. 6 is a graphical representation of circles 3, 4 and 5 of FIG. 3, illustrating the attributes used to determine whether a middle circle should be bypassed.

FIGS. 7A–7F are three-dimensional graphical representations (in six rotations of axis) of the resultant planning volume of a sarcoma.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

It has been found that accurately determining the planning volume of a sarcoma for radiation treatment can maximize local tumor control and minimize normal tissue complications and damage. The present invention is an automated tumor volume contouring algorithm which utilizes computational geometry, numerical interpolation, and artificial intelligence (AI) techniques to determine the planning volume of a sarcoma.

Briefly described, in architecture, one embodiment of the system, among others, can be implemented as follows. By combining both geometric, numerical and AI interpolation techniques, a mathematical algorithm can be used to automatically generate the planning volume of a sarcoma. The planning volume of a sarcoma can be viewed mathematically as the minimum smoothly connected volume that contains a set of "circles." It is envisioned that the automated planning volume algorithm (APVA) system will be implemented in software, hardware or a combination thereof. The algorithms used to determine the planning volume are contingent only upon a series of digitized data inputs. With these inputs, the APVA system automatically calculates an output of digitized coordinates for the planning volume using a configuration of software and hardware. The actual algorithms performing the calculations are essentially a "black box" to the clinician, who merely inputs the data into the system and then evaluates the outputs.

During a surgical procedure, catheters are placed within the tumor bed and a series of images are taken showing the location of the catheters. Indicators are contained in the catheters to identify their positions and the potential positions of the radioactive seeds. To achieve clarity of seed

images and accuracy in seed reconstruction, the patient is positioned so that the catheters are parallel to the gantry axis of rotation of the imaging mechanism. However, in the case where an anatomical site does not allow this, or when the catheters are not all parallel to each other, it is also possible that orthogonal anteroposterior (AP) and lateral films are taken. If there is difficulty in identifying seeds in some of the orthogonal films, oblique film may be needed in order to show all of the seeds. The seed positions are then reconstructed from two films that are less than 90° apart. Although films are mentioned specifically herein, it is envisioned that any means for imaging the sarcoma area may be utilized to provide a pictorial representation of the sarcoma bed and catheter positions.

Catheter and seed positions are reconstructed from the digitization of two films. The algorithm, which “reconstructs” the digital positions for the catheters, compensates for the beam divergence. For every seed position, each film will provide one longitudinal coordinate along the gantry rotation axis. If the patient remains stationary, the longitudinal coordinate will suffice to identify the seed position. However, the patient often moves during the time the two films are acquired; in which case, the final seed position is taken to be the midpoint of the two reconstructed positions. The difference between the two positions defines the localization error, which is normally set to a limit ranging from 0.2 to 0.5 cm. The seed reconstruction is verified by comparing a computer-generated picture of seed positions with the corresponding simulation film. The clinician will determine that the final seed position is acceptable when the localization error is less than approximately 0.2 cm after demagnification.

The target volume, or planning volume, of the sarcoma is defined to be the slab of tissue  $r$  cm perpendicularly away from the curvilinear plane defined by the mesh of catheters. If adjacent catheters are separated by more than  $2r$  cm (or 1 cm), the tissue between the two catheters is assumed to be a part of the tumor bed. The point of intersection of a catheter and a cross-sectional slice is referred to as a “center.” Each center has an associated circle about it with a radius  $r$ . Typically, the radius  $r$  is taken to be 0.5 cm. The input data for the algorithm consists of the digitized coordinates of the catheter positions in each of the cross-sectional slices of the tumor bed and the estimated distance  $r$  from the catheters to the tumor surface.

Mathematically, one can view the planning volume as a minimum smoothly connected surface which contains a set of circles, each circle centered at a given catheter position in a given cross-sectional slice. The algorithm performs local interpolation on consecutive triplets of circles, and returns the planning volume in a matter of minutes.

Viewing each slice as a two-dimensional surface, the algorithm begins by labeling the centers in each slice in a “natural” order. The shape formed by following the associated circles in the specified order provides the overall shape of the tumor bed within the given slice. The algorithm then seeks to form a smoothly connected body that compactly encapsulates the shape of the tumor bed. The algorithm will perform well regardless of whether the catheters are all close together (with the target, a volume mass), the catheters are spread far apart in the plane, or the catheters are arranged in a convoluted way. The performance of the algorithm is measured by the algorithm’s ability to automatically generate clinically acceptable smoothly connected surfaces for anatomical sites of different shapes.

Visually, one can think of the algorithm as constructing an “inner curve” and an “outer curve” tangent to the ordered

collection of circles. Construction of these curves requires the determination of tangent points followed by local interpolation. The algorithm works the same for determining both the outer-curve and inner-curve.

More particularly, the APVA system can be described as a series of algorithmic steps that determine the planning volume of a sarcoma bed from digitized catheter data and a given  $r$ . Following the surgical implantation of catheters into the sarcoma bed, the coordinates of the catheters are digitized and each “sphere” of a specified radius is centered at a given catheter position. The sarcoma bed is then divided into a number of cross-sectional slices. When viewed as cross-sectional slices, the catheter positions are the centers of circles with a specified radius  $r$ . The point of intersection of a catheter and a cross-sectional slice is referred to as a “center,” each of which has a corresponding radius  $r$ .

The digitized coordinates of the catheters and the corresponding radii for each of the cross-sectional slices of the tumor bed comprise the algorithm inputs. The first step of the algorithm is to find the “span” of the circles by locating the two centers, the origin and the destination, that are the furthest apart. Starting at the origin, the algorithm engages in a two-phase procedure of locating and labeling, from left to right, the centers in a “natural” order. The algorithm engages in dynamic local searching and uses a greedy approach to seek out the next-closest center for labeling. If, however, the positions of the catheters and the initial labeling thereof would result in an order of the centers that produces a kink or sharp indentation cutting off part of the sarcoma bed from treatment, the algorithm self-corrects and re-labels and re-orders the centers. Thus, the labeling of the centers and ordering of the circles provides the overall shape of the tumor bed surface.

The second step of the algorithm, the identification of tangent points, is performed after the labeling and ordering step. Based on the order of the centers, tangent points and their corresponding tangent lines are determined for each consecutive pair of circles.

The third step of the algorithm determines whether the middle circle of a group of three consecutive circles may be bypassed. Statistically based artificial intelligence (AI) has shown that the iterations on the circles can sometimes be simplified, and potential kinks removed from the generated curves of the sarcoma surfaces, by removing some of the middle circles from the calculations. For example, if analysis indicates that the middle circle **2** of a triplet of circles **1**, **2** and **3** may be bypassed, the algorithm then proceeds to examine circles **1**, **3** and **4**, wherein circle **3** is now the middle circle, and so forth. Thus, the circles are classified into one of two groups; those circles which may be bypassed or omitted, and those circles which may not be bypassed or must be included in the interpolation. Typically, only a small portion of the circles may be bypassed. The bypassing step is performed twice in conjunction with the local nonlinear interpolation for the inner and outer curves. Thus, a circle may be bypassed in one curve, but included in the other for interpolation purposes.

Following the determination of bypassed circles, step four of the algorithm involves the performance of local nonlinear interpolation on each consecutive pair of tangent lines to give the resultant curved surface of the tumor bed. The interpolation step consists of two phases; a nonintersecting phase, which identifies the non-overlapping tangent line segments, and an intersecting phase, which identifies the intersecting tangent line segments. The local interpolation step is performed twice so as to generate the inner and outer curves of the planning volume for each cross-sectional slice.

The cumulative collection of curves resulting from the local interpolation step specifies the contours of the tumor bed.

From the iterative process of interpolation, the algorithm generates the digitized coordinates and graphical representations that define the planning volume. Finally, the output from the algorithm is evaluated and approved by a clinician.

The present invention can also be viewed as providing methods for mathematically determining the planning volume of sarcoma so as to produce improved brachytherapy treatments. In this regard, one embodiment of such a method, among others, can be broadly summarized by the following steps: insertion of catheters into the sarcoma bed; obtaining a series of images indicating the position of the catheters; digitization of the catheter images; generation of the planning volume and digital positions of the catheters within the planning volume; and comparison of the generated positions with the positions shown on the images. The generation of the planning volume and the digital catheter positions is accomplished with an automatic contouring algorithm comprising an ordering of circles and labeling of circle centers, identification of tangent points, determination of whether middle circles may be bypassed, and local interpolation.

It is anticipated that the Automated Planning Volume Algorithm (APVA) system of the invention can be implemented in software (e.g., firmware), hardware, or a combination thereof. In the currently contemplated best mode, the APVA system is implemented in software, as an executable program, and is executed by a special or general purpose digital computer, such as a personal computer (PC; IBM-compatible, Apple-compatible, or otherwise), workstation, minicomputer, or mainframe computer. As shown in FIG. 1, the APVA system, denoted by reference numeral 10, may be implemented with a general purpose computer.

Generally, in terms of hardware architecture, as shown in FIG. 1, the computer 11 includes a processor 12, memory 14, and one or more input and/or output (I/O) devices 16 (or peripherals) that are communicatively coupled via a local interface 18. The local interface 18 can be, for example but not limited to, one or more buses or other wired or wireless connections, as is known in the art. The local interface 18 may have additional elements, which are omitted for simplicity, such as controllers, buffers (caches), drivers, repeaters, and receivers, to enable communications. Further, the local interface 18 may include address, control, and/or data connections to enable appropriate communications among the aforementioned components.

The processor 12 is a hardware device for executing software that can be stored in memory 14. The processor 12 can be any custom made or commercially available processor, a central processing unit (CPU), an auxiliary processor among several processors associated with the computer 11, a semiconductor based microprocessor (in the form of a microchip or chip set), a macroprocessor, or generally any device for executing software instructions. Examples of suitable, commercially available microprocessors are as follows: a PA-RISC series microprocessor from Hewlett-Packard Company, an 80x86 or Pentium series microprocessor from Intel Corporation, a PowerPC microprocessor from IBM, a Sparc microprocessor from Sun Microsystems, Inc, or a 68APVA series microprocessor from Motorola Corporation. In the preferred embodiment, the APVA system is run on a SUN UltraSparc workstation of 166 MHz.

The memory 14 can include any one or combination of volatile memory elements (e.g., random access memory (RAM, such as DRAM, SRAM, SDRAM, etc.)) and non-volatile memory elements (e.g., ROM, hard drive, tape,

CDROM, etc.). Moreover, the memory 14 may incorporate electronic, magnetic, optical, and/or other types of storage media. Note that the memory 14 may have a distributed architecture, where various components are remotely situated from one another, which can be accessed by the processor 12.

The software in memory 14 may include one or more separate programs, each of which comprises an ordered listing of executable instructions for implementing logical functions. In the example of FIG. 1, the software in the memory 14 includes the APVA system and a suitable operating system (O/S) 22. A non-exhaustive list of examples of suitable commercially available operating systems 22 is as follows: a Windows operating system from Microsoft Corporation, a NetWare operating system available from Novell, Inc., or a UNIX operating system, which is available for purchase from many vendors, such as Hewlett-Packard Company, Sun Microsystems, Inc., and AT&T Corporation. The operating system 22 essentially controls the execution of other computer programs, such as the APVA system 10, and provides scheduling, input-output control, file and data management, memory management, and communication control and related services.

The APVA system 10 is a source program, executable program (object code), script, or any other entity comprising a set of instructions to be performed. As a source program, the program requires translation via a compiler, assembler, interpreter, or the like, which may or may not be included within the memory 14, so as to operate properly in connection with the O/S 22. Furthermore, the APVA system 10 can be written as (a) an object oriented programming language, which has classes of data and methods, or (b) a procedure programming language, which has routines, subroutines, and/or functions, for example but not limited to, C, C++, Pascal, Basic, Fortran, Cobol, Perl, Java, and Ada. In the currently contemplated best mode of the invention, the algorithms for the APVA system 10 are written using the SPLUS 5.0 (Vlathsoft; Seattle, Wash.) language. The series of APVA algorithms are automatically executed by the program to calculate the planning volume of a sarcoma bed from a series of digitized catheter coordinate positions.

The I/O devices 16 may include input devices, for example but not limited to, a keyboard, mouse, scanner, microphone, etc. Furthermore, the I/O devices 16 may also include output devices, for example but not limited to, a printer, display, etc. Finally, the I/O devices 16 may further include devices that communicate both inputs and outputs, for instance but not limited to, a modulator/demodulator (modem; for accessing another device, system, or network), a radio frequency (RF) or other transceiver, a telephonic interface, a bridge, a router, etc.

If the computer 11 is a PC, workstation, or the like, the software in the memory 14 may further include a basic input output system (BIOS) (omitted for simplicity). The BIOS is a set of essential software routines that initialize and test hardware at startup, start the O/S 22, and support the transfer of data among the hardware devices. The BIOS is stored in ROM so that the BIOS can be executed when the computer 11 is activated.

When the computer 11 is in operation, the processor 12 is configured to execute software stored within the memory 14, to communicate data to and from the memory 14, and to generally control operations of the computer 11 pursuant to the software. The APVA system 10 and the O/S 22, in whole or in part, but typically the latter, are read by the processor 12, perhaps buffered within the processor 12, and then executed.

When the APVA system **10** is implemented in software, as is shown in FIG. **1**, it should be noted that the APVA system **10** can be stored on any computer readable medium for use by or in connection with any computer related system or method. In the context of this document, a computer readable medium is an electronic, magnetic, optical, or other physical device or means that can contain or store a computer program for use by or in connection with a computer related system or method. The APVA system **10** can be embodied in any computer-readable medium for use by or in connection with an instruction execution system, apparatus, or device, such as a computer-based system, processor-containing system, or other system that can fetch the instructions from the instruction execution system, apparatus, or device and execute the instructions. In the context of this document, a "computer-readable medium" can be any means that can store, communicate, propagate, or transport the program for use by or in connection with the instruction execution system, apparatus, or device. The computer readable medium can be, for example but not limited to, an electronic, magnetic, optical, electromagnetic, infrared, or semiconductor system, apparatus, device, or propagation medium. More specific examples (a non-exhaustive list) of the computer-readable medium would include the following: an electrical connection (electronic) having one or more wires, a portable computer diskette (magnetic), a random access memory (RAM) (electronic), a read-only memory (ROM) (electronic), an erasable programmable read-only memory (EPROM, EEPROM, or Flash memory) (electronic), an optical fiber (optical), and a portable compact disc read-only memory (CDROM) (optical). Note that the computer-readable medium may also include paper or another suitable medium upon which the program is printed, since the program is electronically captured, via for instance optical scanning of the paper or other medium, and then compiled, interpreted or otherwise processed in a suitable manner, if necessary, for storage in a computer memory.

In an alternative embodiment, where the APVA system **10** is implemented in hardware, the APVA system can be implemented with any or a combination of the following technologies, which are each well known in the art: a discrete logic circuit(s) having logic gates for implementing logic functions upon data signals, an application specific integrated circuit (ASIC) having appropriate combinational logic gates, a programmable gate array(s) (PGA), a field programmable gate array (FPGA), etc.

FIG. **2A** illustrates one possible configuration of an imaging device **62**, for inputting data **26** (i.e. catheter coordinates), with a computer **11**, and further illustrates the APVA program **10** and the steps performed thereby to generate the planning volume **42**. Particularly, the APVA program **10** will perform an initial step of Obtaining the Inputted Catheter Coordinates **64** for analysis. From the input data **26**, the program **10** will Determine the Span **66** (or furthest distance between the centers), Label the Circle Centers **68**, and Order the Circles **70** into a natural order. Cumulatively these steps (**66**, **68** and **70**) comprise the labeling circle centers and ordering of circles algorithm **28** (see FIG. **2B**). Next, a certain radius  $r$  is defined about each center **72**. With the dimensions of the circles defined, tangent points are identified along the circles **74** and therefrom tangent lines **76** are identified; referred to as the algorithm for Tangent Point Identification **30** (see FIG. **2B**). The APVA program **10** then determines the distances between each circle in consecutive triplets of circles **78** in order to ascertain whether a middle circle of each consecutive triplet of circles may be bypassed **80** for a particular interpolation. Together steps **78** and **80**

comprise the Determine Bypassing Circles algorithm **32** (see FIG. **2B**). For interpolation, the tangent lines are separated into intersecting and non-intersecting tangent lines. Interpolation is performed on non-intersecting tangent lines **82** and interpolation is also performed on intersecting tangent lines **84**, the cumulative curve formed by the interpolation steps is determined in accordance with the Local Interpolation algorithm **34** (see FIG. **2B**). Finally, the interpolation data for both inner and outer curves of all cross-sectional slices is combined **86** to generate the planning volume and is outputted in the form of digitized coordinates and graphics **88**.

As shown in FIG. **2B**, the APVA system **10** consists of a series of algorithms which utilize the input data **26** (i.e. digitized catheter coordinates) to calculate the planning volume **42**. The steps of the APVA system **10** include Ordering of Circles **28**, the Identification of Tangent Points **30**, the Determination of Bypassed Circles **32**, and Local Interpolation **34**. These steps occur in essentially a "black box" **40** and are automatically calculated by the APVA algorithms. The output **36** (i.e. digitized coordinates and graphics showing the planning volume) is thus automatically generated by the APVA system **10** from the input data **26**. The output **36** is evaluated and approved during a clinician review **38**.

FIG. **3** illustrates a cross-sectional slice **41** of a soft-tissue sarcoma on the left shoulder of a patient. The catheters inserted during surgery are shown as centers **44** (numbers **1-9**) in the cross-sectional slice **41**. Around each center **44**, a radius  $r$  **46** is drawn which represents the target volume as a circle **43**. The algorithm begins by determining the "span" **50** of the circle **43** centers **44**. The centers **44** are labeled from left to right, starting at the origin and proceeding in natural order to the destination **49**. Tissue between adjacent catheters that are more than approximately 1 cm apart is considered part of the tumor bed. In the preferred embodiment, the Labeling Circle Centers and Ordering of Circles **28** is conducted in accordance with the following:

Let  $n$  be the number of centers **44** on a cross-sectional slice **41**, where  $p$  is the parent circle center,  $i$  is an indexer,  $a_{nil}$  indicates that the circle center has not been labeled and has no parent,  $t$  is an indexer,  $lastindex$  indicates the last index used,  $tmpindex$  indicates a temporary storage index,  $d$  is a destination and  $c_k$  is the center of the circle that has not been labeled. Assume the centers **44** of the circles **43** are ordered as  $c_1, \dots, c_n$ . Denote the circle **43** corresponding to center **44**  $c_i$  by  $C_i$ .

1. Initialization: Set  $N = \{1, \dots, n\}$ ;  $p[i] = nil$  for all  $i \in N$ ;  $a_{nil} =$ ;  $lastindex = 0$ ;  $L = \{0\}$ ;  $L = N \setminus L$ ;  $t = 1$ .
2. Iteration  $t$ : Find  $i \in L$  such that  $a_i$  is closest in Euclidean distance from center  $a_{lastindex}$ . If  $a_{p[lastindex]} - a_i > a_{[lastindex]} - a_i$ , set  $p[i] = lastindex$ . Otherwise, set  $p[i] = p[lastindex]$ ,  $tmpindex = p[lastindex]$ ,  $p[lastindex] = p[tmpindex]$ ,  $p[tmpindex] = lastindex$ .
3. Update:  $L = L \setminus \{i\}$ ,  $t = t + 1$ ,  $lastindex = i$ . If  $L = 0$ , or if  $lastindex = d$ , go to step 4. Otherwise, go to step 2.
4. Constructing the labels: Recover the sequence of centers by using  $p$  to backtrack. Call the recovered sequence  $c_1, \dots, c_{|L|}$  (Here,  $|L|$  denotes the number of elements in the set  $L$ .)

If  $L = 0$ , labeling is complete. Otherwise,  $|L|$  centers, represented by  $c_1, \dots, c_{|L|}$  have been labeled and proceed to second-stage correction for the remaining  $n - |L|$  centers in order to verify that all centers have been included. For each remaining center  $a_i$ ,  $i \in L$ , the correction algorithm selects among the labeled centers the one,  $c_k$ , that is closest to  $a_i$ .

The center  $a_i$  is then inserted either between  $c_{k-1}$  and  $c_k$  or between  $c_k$  and  $c_{k+1}$ , depending on the distance of  $a_i$  from  $c_{k-1}$  and  $c_{k+1}$ .

After the centers **44** have been ordered and labeled (i.e. the ordering and labeling of circles **28** as shown in FIG. 2B), the second step of the APVA system **10** is the identification of tangent points **30**. FIG. 4 focuses on the **3**, **4** and **5** circles **43** of FIG. 4. In the identification of tangent points **30** step, the algorithm constructs tangent points **52** along the circles **43**. These tangent points **52** correspond to tangent lines **53**. In FIG. 3, the tangent points **52**,  $t_3$  and  $t_3'$ , on **3** and **4** circles **43** are shown. Some of the tangent points **52** are later used as the interpolation points **54** in the local interpolation step **34**. The tangent point identification **30** is accomplished by the following:

For each consecutive pair of circles **43**,  $C_i$  and  $C_{i+1}$ , identify a point  $t_i$  on  $C_i$  and a point  $t_i'$  on  $C_{i+1}$  such that the line segment connecting  $t_i$  and  $t_i'$  is tangent to both circles **43** and parallel to the line segment connecting  $C_i$  and  $C_{i+1}$ , i.e. the tangent line segment **53**,  $l_i$  of  $C_i$  and  $C_{i+1}$ . The tangent point identification **30** step requires exactly  $2(n-1)$  operations to complete.

Having established the tangent points **52** and tangent lines **53** for the circles **43**, the algorithm then determines whether certain circles **43** may be bypassed for iterations of local interpolation **34** (the determine bypassing circles **32** step (see FIG. 2B)). Each circle **43**, out of consecutive triplets of circles **57**, is examined to determine if it should be included in the interpolation step **34**. FIG. 6 illustrates an instance in which a circle **43** can be bypassed due to the attributes **58** of the spatial relationship between the **3**, **4** and **5** circles **43**. The attributes **58** indicate the distances between the circles **43** and are labeled as  $d1$ ,  $d2$ ,  $d3$  and  $d4$  in FIG. 6. It is shown that the middle circle **59**, denoted as circle **4**, is bypassed, and that the **3** and **5** circles **43** are included for iterative purposes of local interpolation **34**. The algorithm then proceeds to analyze the **3**, **5** and **6** circles **43** to determine if the “new” middle circle **59** may be bypassed. Whether a circle **43** may be bypassed **32** is determined in accordance with the following:

The current circle,  $C_{i+1}$  (or circle **4** on FIG. 6), is viewed in relation to circles  $C_i$  and  $C_{i+2}$ , where  $C_i$  is the highest labeled circle in the sequence not bypassed thus far. For  $i=1, \dots, n-2$  triplets of circles **57**,  $C_i$ ,  $C_{i+1}$  and  $C_{i+2}$ , artificial intelligence and machine learning techniques are used to designate which circles **43** may be bypassed. Associated with the circles  $C_i$ ,  $C_{i+1}$  and  $C_{i+2}$ , are tangent points  $t_3'$  and  $t_4$ . If the distance between  $C_i$  and  $C_{i+1}$  and the distance between  $C_{i+1}$  and  $C_{i+2}$  are both less than  $2r$ , and the associated tangent points  $t_3'$  and  $t_4$  are within  $r$ , then the middle circle **59** is bypassed.

Once the algorithm has determined which circles **43** are to be bypassed **32**, the circles **43** are separated into groups of bypassed or non-bypassed circles. The circles **43** that are bypassed are not included in the interpolation step **34** and the circles **43** that are not bypassed are included in the interpolation step **34**, such that a smooth curve is maintained for both the inner **60** and outer **61** curves of the planning volume **42**. The bypassing step **32** is performed twice in conjunction with the local nonlinear interpolation **34** for the inner **60** and outer **61** curves. Thus, a circle **43** may be bypassed in one curve, but included in the other for interpolation purposes.

The algorithm then performs local interpolation **34** on the consecutive triplets of circles **57**, with the last circle **43** of one iteration serving as the first circle **43** of the next iteration. In this manner, the local nonlinear interpolation **34** is performed on consecutive pairs of tangent lines **53** in two

phases, the non-intersecting phase and the intersecting phase. In the non-intersecting phase, the non-intersecting tangent line **54** segments are identified and the curve is constructed in accordance with the following:

For consecutive triplets of tangent lines **53**,  $l_i$ ,  $l_{i+1}$ , and  $l_{i+2}$ , if  $l_i$  does not intersect  $l_{i+1}$  and  $l_{i+1}$  does not intersect  $l_{i+2}$ , then  $l_{i+1}$ , plus the arc in the middle circle **59** becomes part of the resulting curve for non-intersecting tangent line phase. The next iteration continues using the tangent lines **53**  $l_{i+1}$ ,  $l_{i+2}$ , and  $l_{i+3}$ . FIG. 5 illustrates a non-intersecting iteration on the **3**, **4** and **5** circles **43**.

In the intersecting phase, the pairs of consecutive intersecting tangent line segments **55** are identified and the curve is constructed in accordance with the following:

For every consecutive pair of tangent lines **53**,  $l_i$  and  $l_{i+1}$ , that intersect, nonlinear interpolation is performed using one point (interpolation point **54**) on each tangent line **53** and their intersection point. Specifically, recall  $t_i$  and  $t_i'$  are the tangent points **52** for  $l_i$  on circles  $C_i$  and  $C_{i+1}$ , respectively. If  $l_i$  does not intersect with  $l_{i-1}$ , then  $t_i$  will be chosen for interpolation for tangent line **53**  $l_i$ , otherwise, the mid-point between  $t_i$  and  $t_i'$  will be used. Similarly, if  $l_{i+1}$  does not intersect with  $l_{i+2}$ , then  $t_{i+1}'$  will be used. Otherwise, the midpoint of  $t_i'$  and  $t_{i+1}'$  will be employed. The curve obtained from the interpolation constitutes the curve for the tumor surface around these circles **43**. FIG. 5 illustrates an intersecting iteration on the **2**, **3** and **4** circles **43**.

The iterations will continue until  $C_n$  is employed in the interpolation, at which point the iteration should stop. It is possible that the final iteration will include only two circles **43** for a local interpolation **34**, in which case the local curve is simply the tangent line **53** connecting the two circles **43**.

The local interpolation **34** step is performed twice so as to generate the inner **60** and outer **61** curves (see FIG. 3) along the circles **43** of the planning volume for each cross-sectional slice **41**. The cumulative collection of curves **60**, **61** resulting from the local interpolation **34** step specifies the contours of the tumor bed. From the iterative process of interpolation, the algorithm generates, without any human intervention, an output **36** consisting of the digitized coordinates and graphics which define the planning volume **42** for each slice **41**. Examples of the three dimensional graphical output of the planning volume **42**, rotated through six axis, are shown in FIGS. 7A–7F. Finally, the output **36** from the APVA algorithm **10** is evaluated and approved by a clinician (see **38** on FIG. 2B).

It should be emphasized that the above-described embodiments of the present invention, particularly, any “preferred” embodiments, are merely possible examples of implementations, merely set forth for a clear understanding of the principles of the invention. Many variations and modifications may be made to the above-described embodiment(s) of the invention without departing substantially from the spirit and principles of the invention. All such modifications and variations are intended to be included herein within the scope of this disclosure and the present invention and protected by the following claims.

Therefore, having thus described the invention, at least the following is claimed:

**1.** A computer readable medium having computer-executable instructions for automatically determining a planning volume of a sarcoma said computer-executable instructions, comprising:

means for locating catheter coordinates for catheters inserted into the sarcoma, where the catheters are configured as centers in cross-sectional slices of the sarcoma;

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means for inputting the catheter coordinates;  
 means for selecting circles of radius  $r$  about the centers;  
 means for labeling the centers and ordering the circles;  
 means for identifying tangent points and corresponding  
 tangent lines;  
 means for determining whether a circle should be  
 included in or omitted from interpolation to determine  
 the planning volume;  
 means for performing local interpolation on the circles;  
 means for generating digital coordinates and graphical  
 outputs showing the planning volume; and  
 means for evaluating the planning volume outputs.

2. The computer readable medium of claim 1, wherein the  
 means for locating catheter coordinates for catheters inserted  
 into the sarcoma comprises the use of an imaging device to  
 generate a series of films showing the positions of the  
 catheters within the sarcoma.

3. The computer readable medium of claim 2, further  
 comprising the digitization of the catheter coordinates.

4. The computer readable medium of claim 1, wherein the  
 means for selecting circles of radius  $r$  about the centers  
 further comprises selecting the radii such that the circles  
 substantially cover surfaces of the cross-sectional slices of  
 the sarcoma.

5. The computer readable medium of claim 1, wherein the  
 means for labeling of centers and ordering of circles com-  
 prises an algorithm having four phases, the phases consist-  
 ing of initialization, iteration  $t$ , update and construction of  
 labels, and is of the formula:

Initialization: Set  $N=\{1, \dots, n\}$ ;  $p[i]=\text{nil}$  for all  $i \in N$ ;  
 $a_{\text{nil}}=\infty$ ,  $\text{lastindex}=0$ ;  $L=\{0\}$ ;  $L=N \setminus L$ ;  $t=1$ ;

Iteration  $t$ : Find  $i \in L$  such that  $a_i$  is closest in Euclidean  
 distance from center  $a_{\text{lastindex}}$ . If  $\|a_{p[\text{lastindex}]}-a_i\| >$   
 $\|a_{\text{lastindex}}-a_i\|$ , set  $p[i]=\text{lastindex}$ . Otherwise, set  $p[i]=p$   
 $[\text{lastindex}]$ ,  $\text{tmpindex}=p[\text{lastindex}]$ ,  $p[\text{lastindex}]=p$   
 $[\text{tmpindex}]$ ,  $p[\text{tmpindex}]=\text{lastindex}$ ;

Update:  $L \leftarrow L \setminus \{i\}$ ,  $t \leftarrow t+1$ ,  $\text{lastindex}=i$ . If  $L=0$ , or if  
 $\text{lastindex}=d$ , go to Construction of labels. Otherwise,  
 go to iteration  $t$ ;

Construction of labels: Recover the sequence of centers  
 by using  $p$  to backtrack, the recovered sequence being  
 $c_i, \dots, c_L$ ;

where  $n$  is the number of centers on the cross-sectional slice,  
 $p$  is the parent circle center,  $i$  is an indexer,  $a_{\text{nil}}$  indicates that  
 the circle center as not been labeled and has no parent,  $t$  is  
 an indexer,  $\text{lastindex}$  indicates the last index used,  $\text{tmpindex}$   
 indicates a temporary storage index,  $d$  is a destination,  $c_k$  is  
 the center of the circle that has not been labeled, and where  
 the centers of the circles are ordered as  $c_1, \dots, c_n$ , and the  
 circles corresponding to the centers are denoted as  $C_i$ , and  $|L|$   
 denotes the number of elements in the set  $L$ .

6. The computer readable medium of claim 5, wherein if  
 $L=0$ , labeling of the centers and ordering of the circles is  
 complete.

7. The computer readable medium of claim 5, wherein if  
 $L \neq 0$ , the labeling and ordering algorithm performs a sec-  
 ond-stage correction for centers  $n-L$  wherein a remaining  
 center  $a_i$ ,  $i \in L$ , is inserted between the closer of  $(c_{k-1}$  and  $c_k)$   
 or  $(c_k$  and  $c_{k+1})$ .

8. The computer readable medium of claim 1, wherein the  
 means for identifying tangent points and corresponding  
 tangent lines comprises a mathematical determination of a  
 tangent point on each of a consecutive pair of circles.

9. The computer readable medium of claim 8, further  
 comprising instructions for determination of the tangent  
 points such that a resultant line segment connecting the

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tangent points is tangent to both of the circles and parallel to  
 a line segment connecting the circles.

10. The computer readable medium of claim 1, wherein  
 the means for determining whether a circle should be  
 included in or omitted from interpolation to determine the  
 planning volume comprises an algorithm which examines  
 distances between each circle in a consecutive triplet of  
 circles.

11. The computer readable medium of claim 10, further  
 comprising instructions for the omission of the middle circle  
 from the interpolation where:

the distance between the middle circle and each of the  
 other two circles of the triplet of circles is less than  $2$   
 $r$ ; and

the distance between the middle circle and tangent points  
 of the triplet of circles is less than  $r$ .

12. The computer readable medium of claim 1, wherein  
 the means for interpolation on the circles comprises an  
 interpolation algorithm performing iterations on consecutive  
 triplets of circles.

13. The computer readable medium of claim 12, wherein  
 the iterations are performed such that a last circle of one  
 iteration serves as a first circle of a next iteration.

14. The computer readable medium of claim 12, further  
 comprising instructions for:

performance of the local interpolation on consecutive  
 pairs of tangent lines, the tangent lines corresponding  
 to the consecutive triplets of circles; and

performance of the local interpolation in an intersecting  
 phase and a non-intersecting phase.

15. The computer readable medium of claim 14, wherein  
 the non-intersecting phase comprises:

identification of tangent line segments that do not inter-  
 sect;

constructing a curve from the non-intersecting tangent  
 line segments and a portion of an arc in a middle circle  
 of the triplet of circles.

16. The computer readable medium of claim 14, wherein  
 the intersecting phase comprises:

identification of tangent line segments that do intersect;  
 performing nonlinear interpolation using a point from  
 each of the intersecting tangent line segments and the  
 point of intersection of the intersecting tangent line  
 segments; and

constructing a curve from the interpolation which consti-  
 tutes the curve around the triplet of circles.

17. The computer readable medium of claim 1, wherein  
 the means for interpolation on the circles comprises an  
 interpolation algorithm performing iterations on consecutive  
 triplets of circles, and further comprising:

performing the local interpolation a first time to construct  
 an inner curve along the circles;

performing the local interpolation a second time to con-  
 struct an outer curve along the circles; and

combining the inner and outer curves so as to specify the  
 planning volume of the sarcoma.

18. The computer readable medium of claim 1, wherein  
 the means for generating digital coordinates and graphical  
 outputs showing the planning volume comprise a conversion  
 of mathematical data into pictorial representations of the  
 planning volume and locations of the catheters.

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19. The computer readable medium of claim 1, wherein the means for evaluating the planning volume outputs comprise review and evaluation of digital coordinates and graphical data by a clinician.

20. A computer readable medium for automatically determining planning volumes of sarcomas for brachytherapy treatment, comprising:

logic configured to receive digital input data relating to a catheter coordinate that defines the location of a radiation dispensing catheter; and

logic configured to execute a geometric algorithm from the input data, to automatically determine a planning volume of a sarcoma.

21. The computer readable medium of claim 20, wherein the logic configured to determine the planning volume further comprises:

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logic configured to construct at least one circle from a cross-section of the sarcoma, wherein the circle is centered around the catheter, and has a predefined radius;

logic configured to construct at least one tangent line on each circle that comprises the planning volume;

logic configured to determine whether any circle may be bypassed, based on the spatial relationship between consecutive circles; and

logic configured to generate contours of the planning volume.

22. The computer readable medium of claim 20, wherein the planning volume is derived from a tumor bed.

\* \* \* \* \*

UNITED STATES PATENT AND TRADEMARK OFFICE  
**CERTIFICATE OF CORRECTION**

PATENT NO. : 7,107,089 B2  
APPLICATION NO. : 10/465341  
DATED : September 12, 2006  
INVENTOR(S) : Eva K. Lee

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

Title page of patent, item (73): add --Emory University, Atlanta, GA (US)-- starting on the line beneath "Atlanta, GA (US)".

Column 3, line 47 – omit the comma after "Instead".

Column 5, line 36 – omit space between "2" and "r".

Column 10, line 41 – "as" should be replaced with --has--.

Column 11, line 8 – "FIG. 4" should be replaced with --FIG. 3--.

Column 11, line 11 – "FIG. 3" should be replaced with --FIG. 4--.

Column 11, line 49 – omit space between "2" and "r".

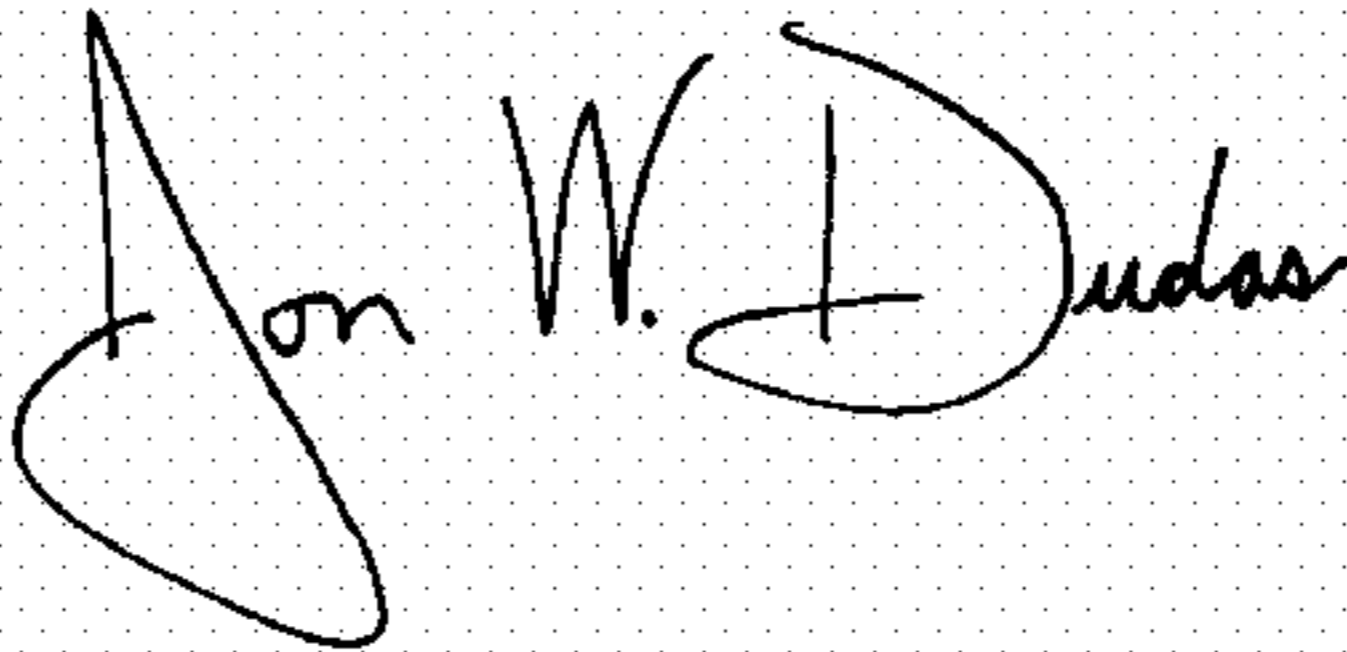
Column 12, line 62 – add a comma between "sarcoma" and "said" and omit the comma after "instructions".

Column 13, line 46 – replace "as" with --has--.

Column 14, lines 14 and 15 – omit the space between "2" and "r".

Signed and Sealed this

Eleventh Day of September, 2007

A handwritten signature in black ink on a light gray dotted background. The signature reads "Jon W. Dudas" in a cursive style.

JON W. DUDAS

*Director of the United States Patent and Trademark Office*