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**Bouton**

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(54) **SCANNING SYSTEM AND METHOD FOR LOCATING SOURCES OF RADIATION EMISSION**

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(52) **U.S. Cl.** ..... **600/436; 250/336.1; 250/370.01**

(58) **Field of Search** ..... **600/407, 436; 250/370.06, 370.08, 370.09**

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| 4,889,991 | 12/1989 | Ramsey et al. .      |
| 4,893,013 | 1/1990  | Denen et al. .       |
| 5,070,878 | 12/1991 | Denen .              |
| 5,151,598 | 9/1992  | Denen .              |
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| 5,383,456 | 1/1995  | Arnold et al. .      |
| 5,429,133 | 7/1995  | Thurston et al. .    |
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| 5,482,040 | 1/1996  | Martin, Jr. .        |
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Morton, et al. "Technical Details of Intraoperative Lymphatic Mapping for Early Stage Melanoma," *Arch. Surg.* 1992; 127: 392-399.

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Cote, et al., "Intraoperative Detection of Occult Colon Cancer Micrometastases Using 125I-Radiolabeled Monoclonal Antibody CC49," *Cancer* 1996; 77:613-620.

*Primary Examiner*—Marvin M. Lateef

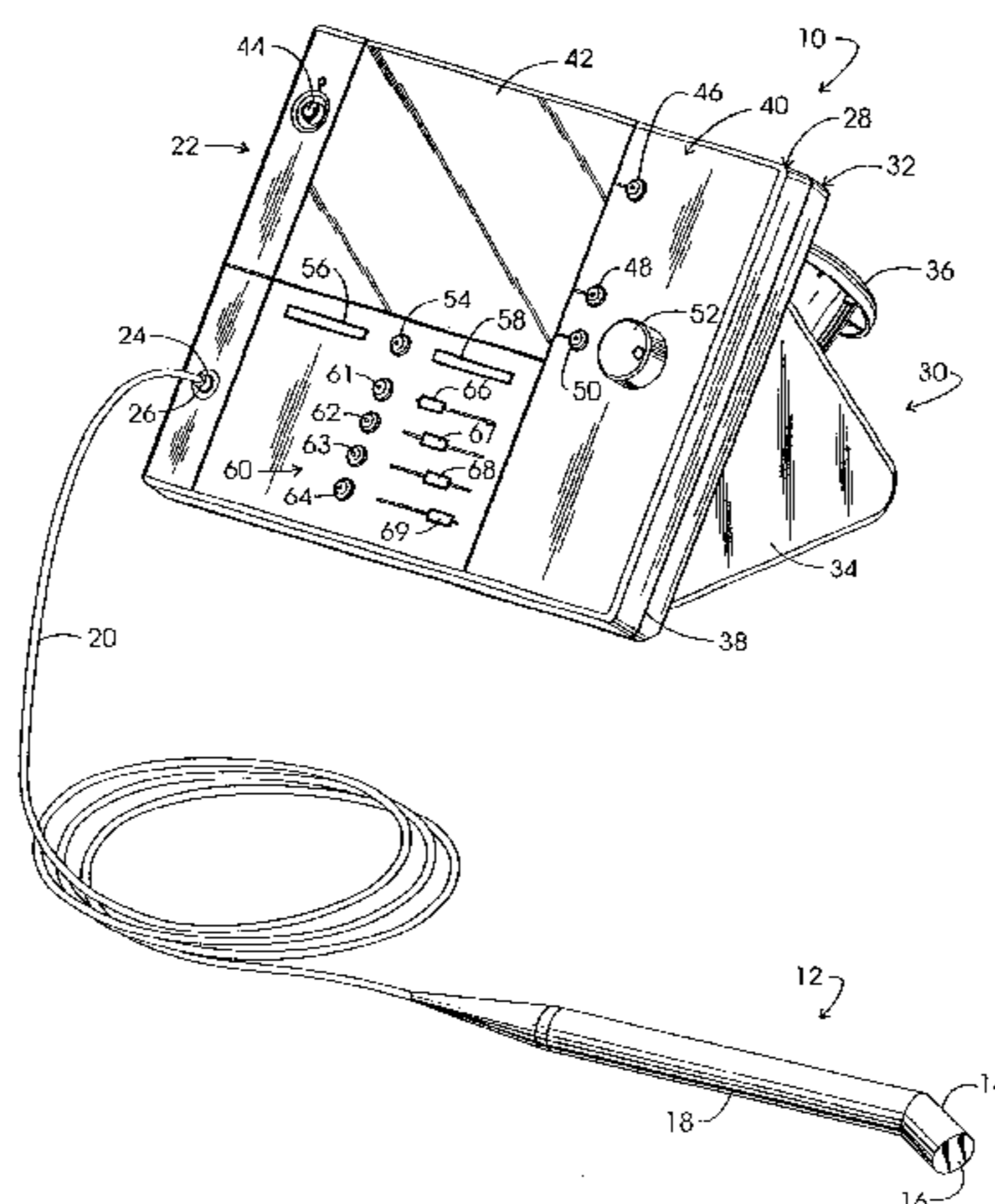
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(57) **ABSTRACT**

A scanning system for a hand-held probe employs a 50 ms scanning interval in conjunction with circular memory. Combinations of segment bins from the circular memory are acquired following each short scanning interval. A threshold is computed for each combination initially based upon a threshold factor which is statistically significant and has a value of three. Audible cueing is developed if any three of six of these combinations of segment bin scan counts exceeds a correspondingly computed threshold value. Thereafter, the threshold factor is diminished to a value of one and the same thresholding tests are carried out to maintain audible cueing. Running count rates are computed as the average of the entire circular buffer memory divided by its corresponding total collection time. This computation is provided on a one half second updated basis.

**31 Claims, 14 Drawing Sheets**



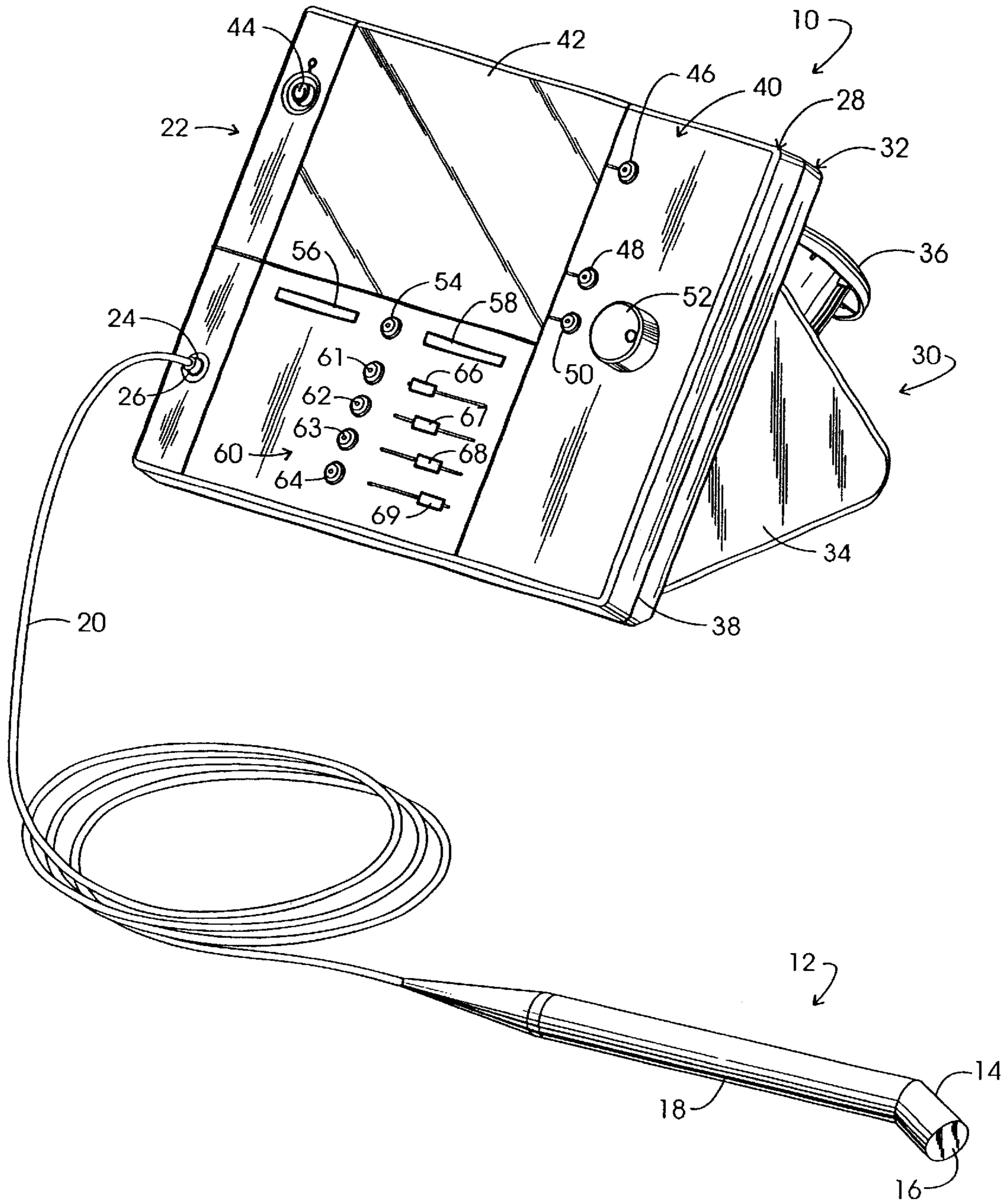


FIG. 1

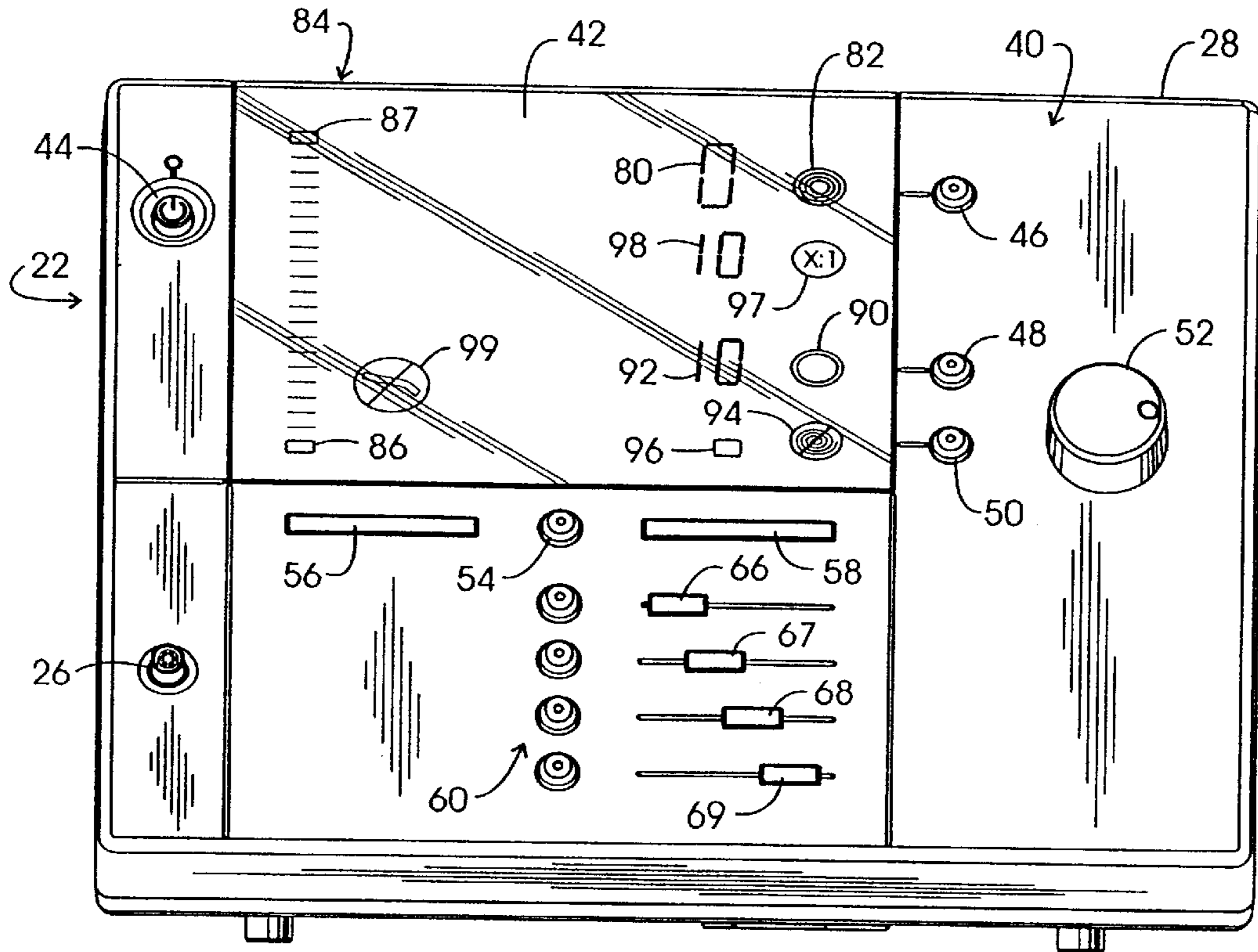


FIG. 2

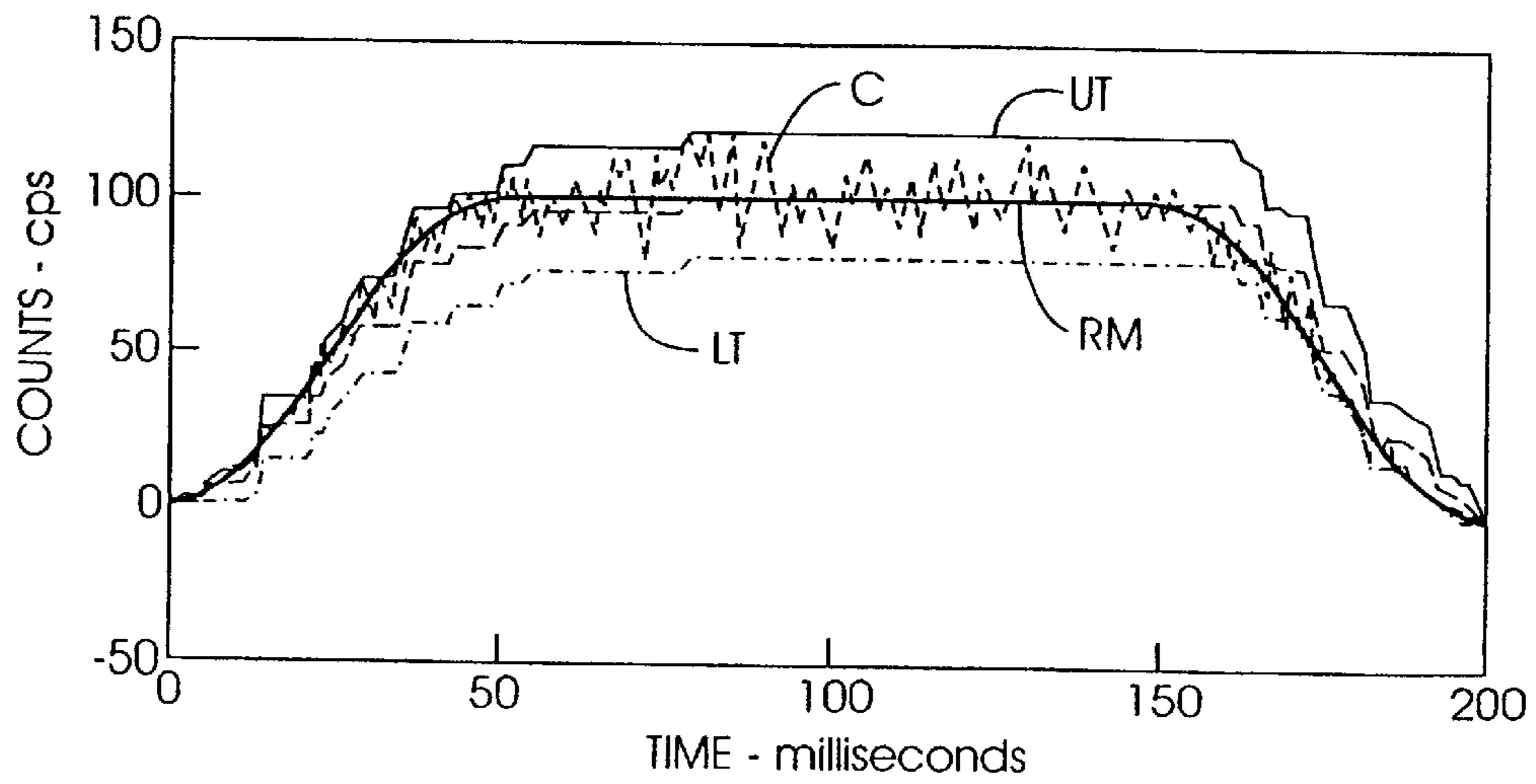
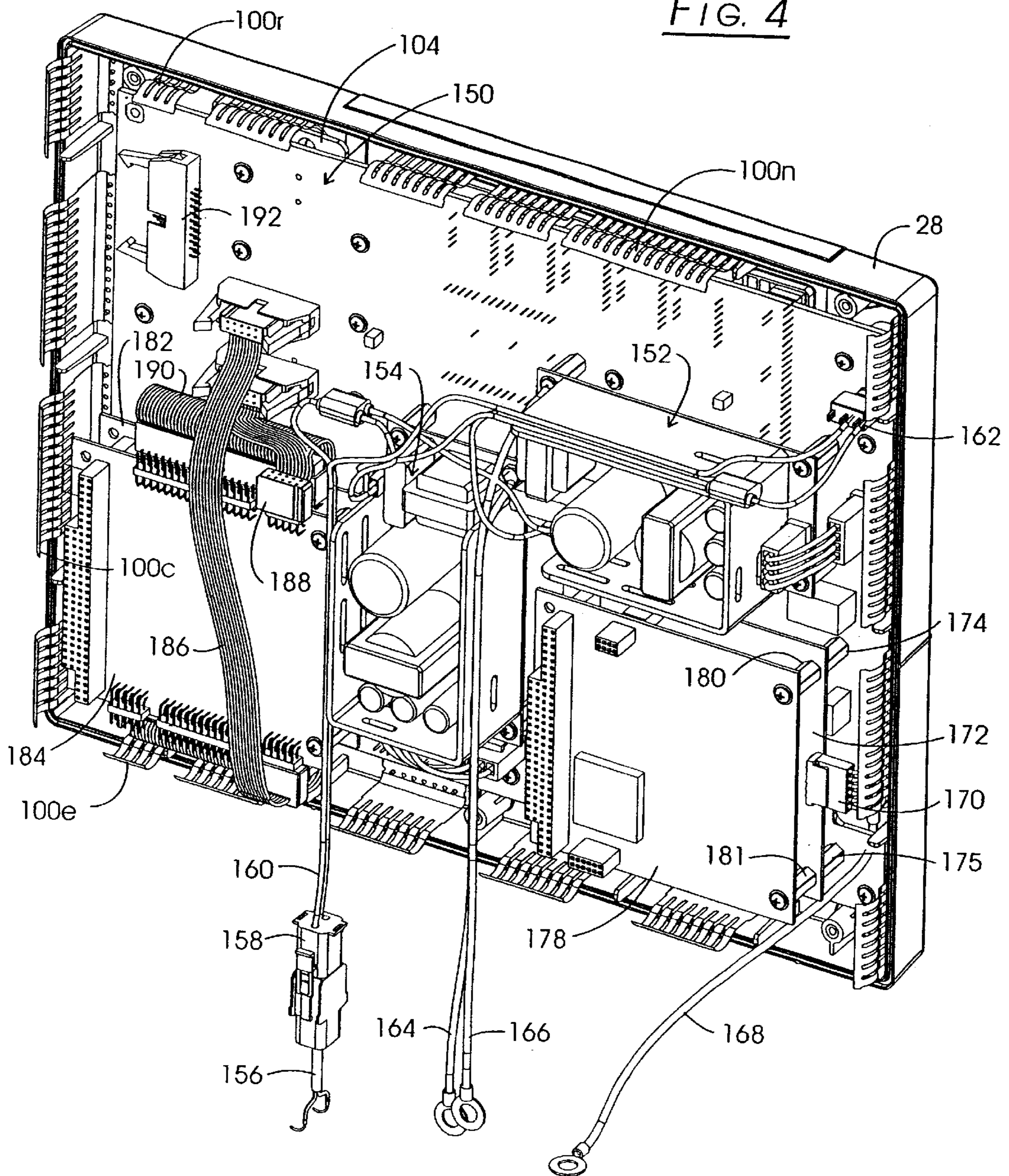


FIG. 7



FIG. 4





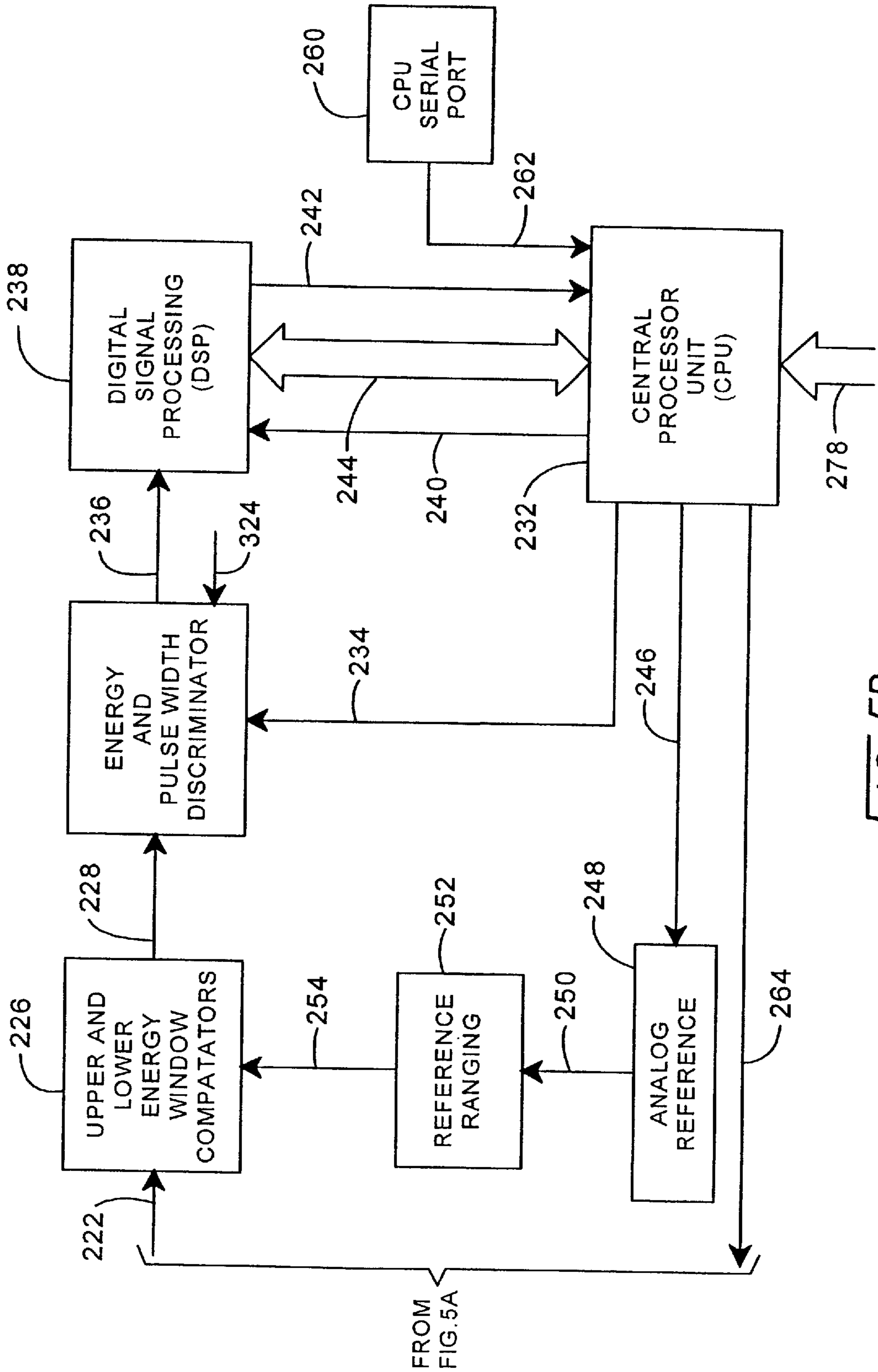


FIG. 5B

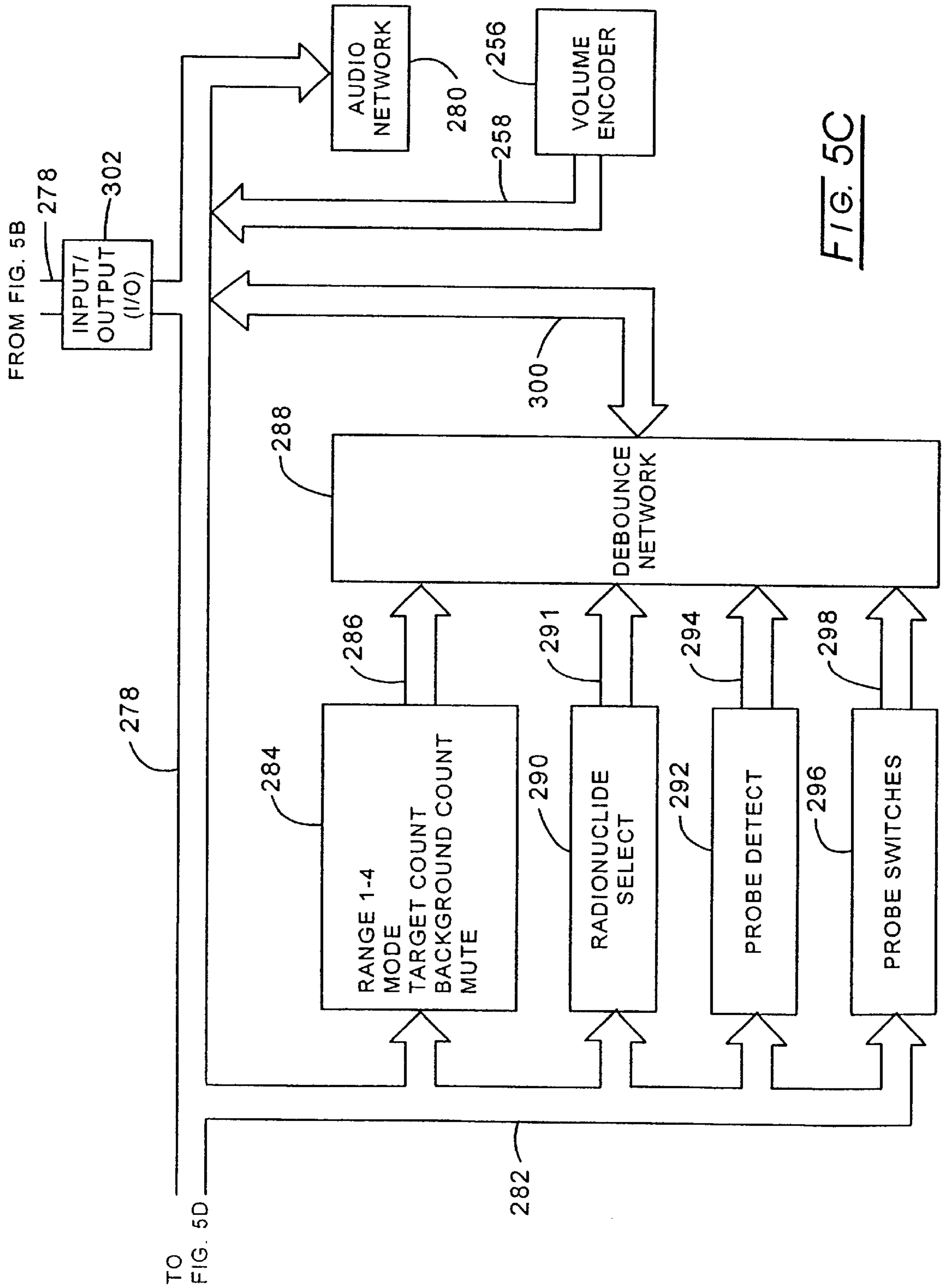


FIG. 5C



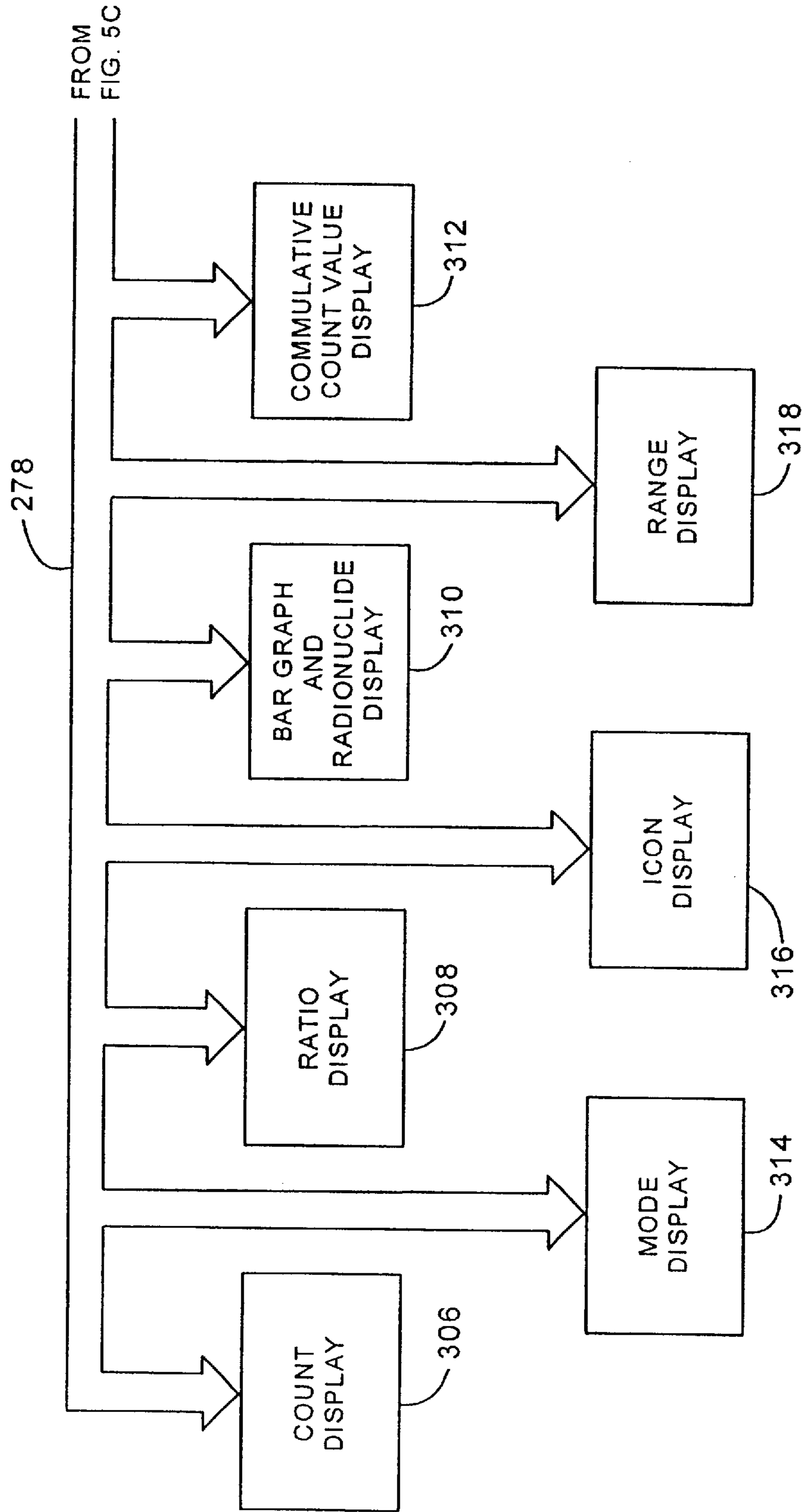
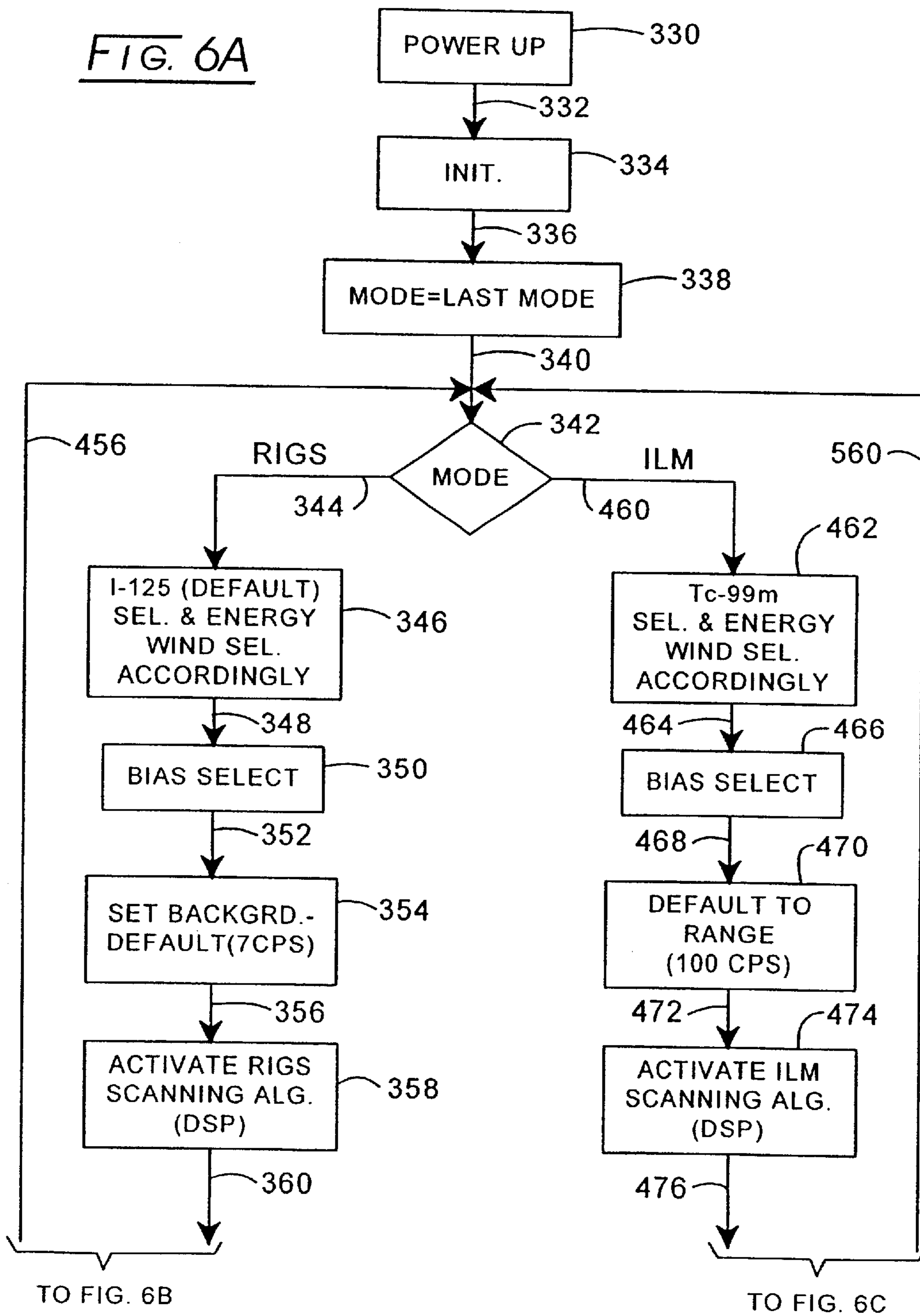
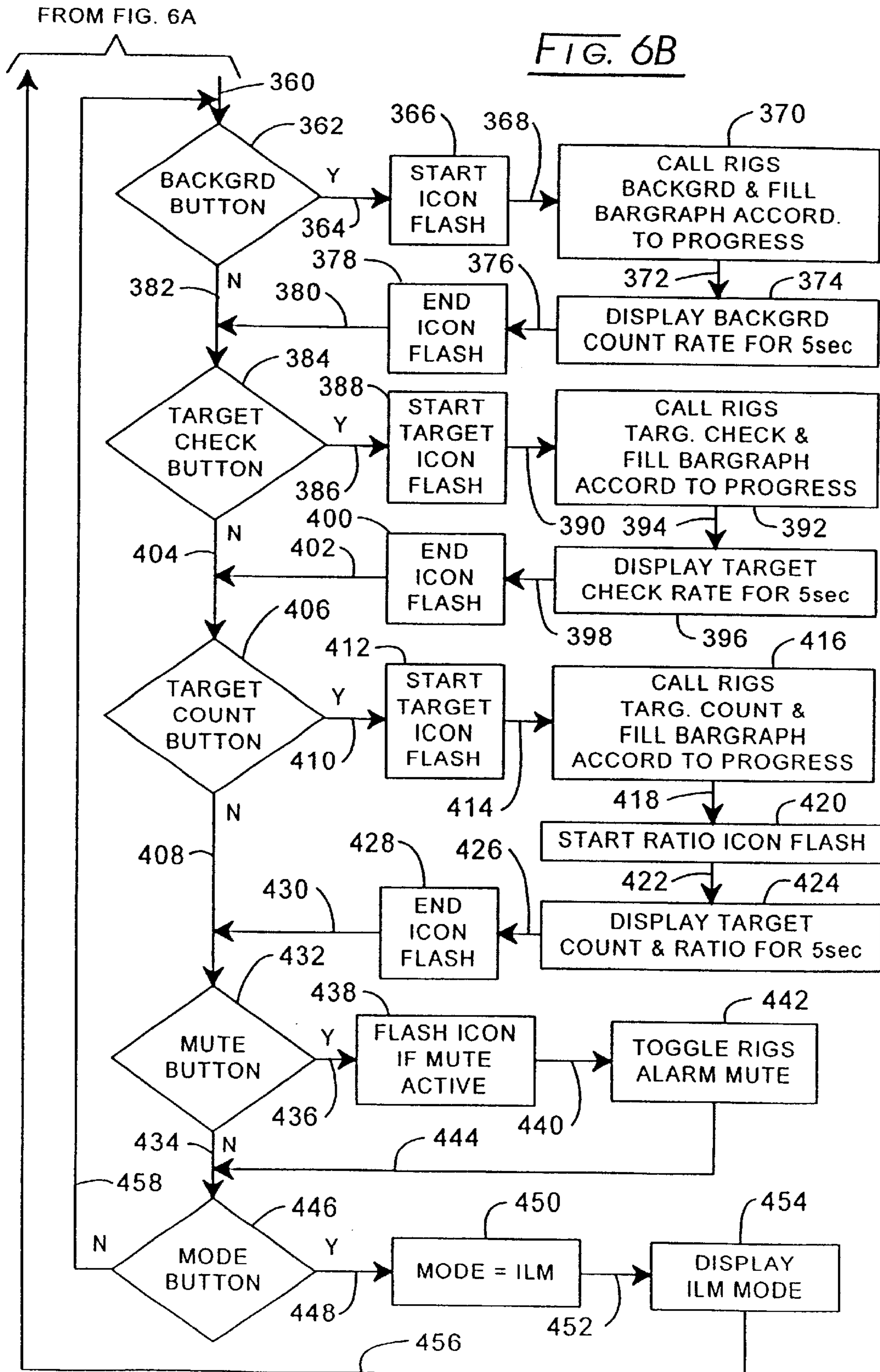
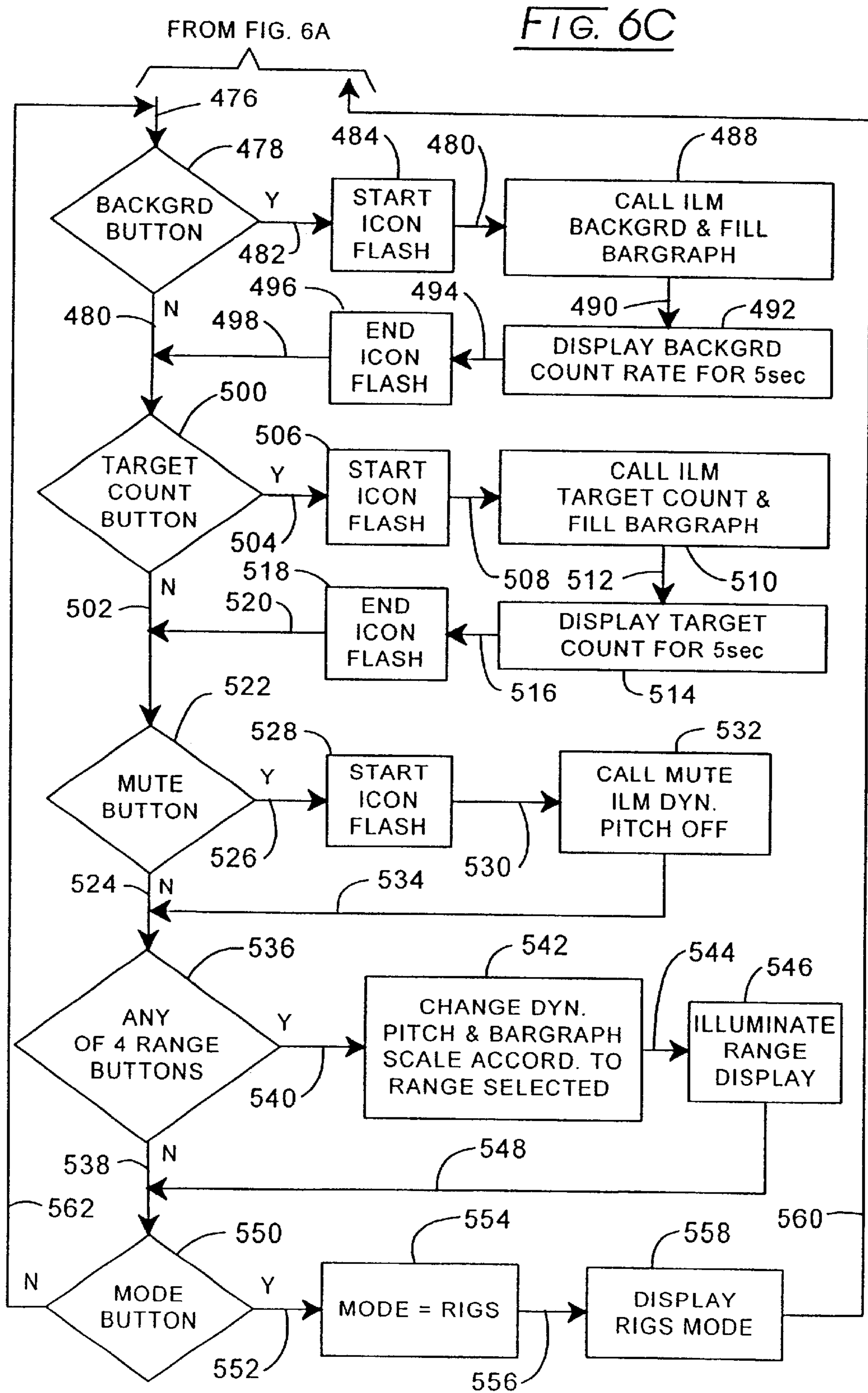


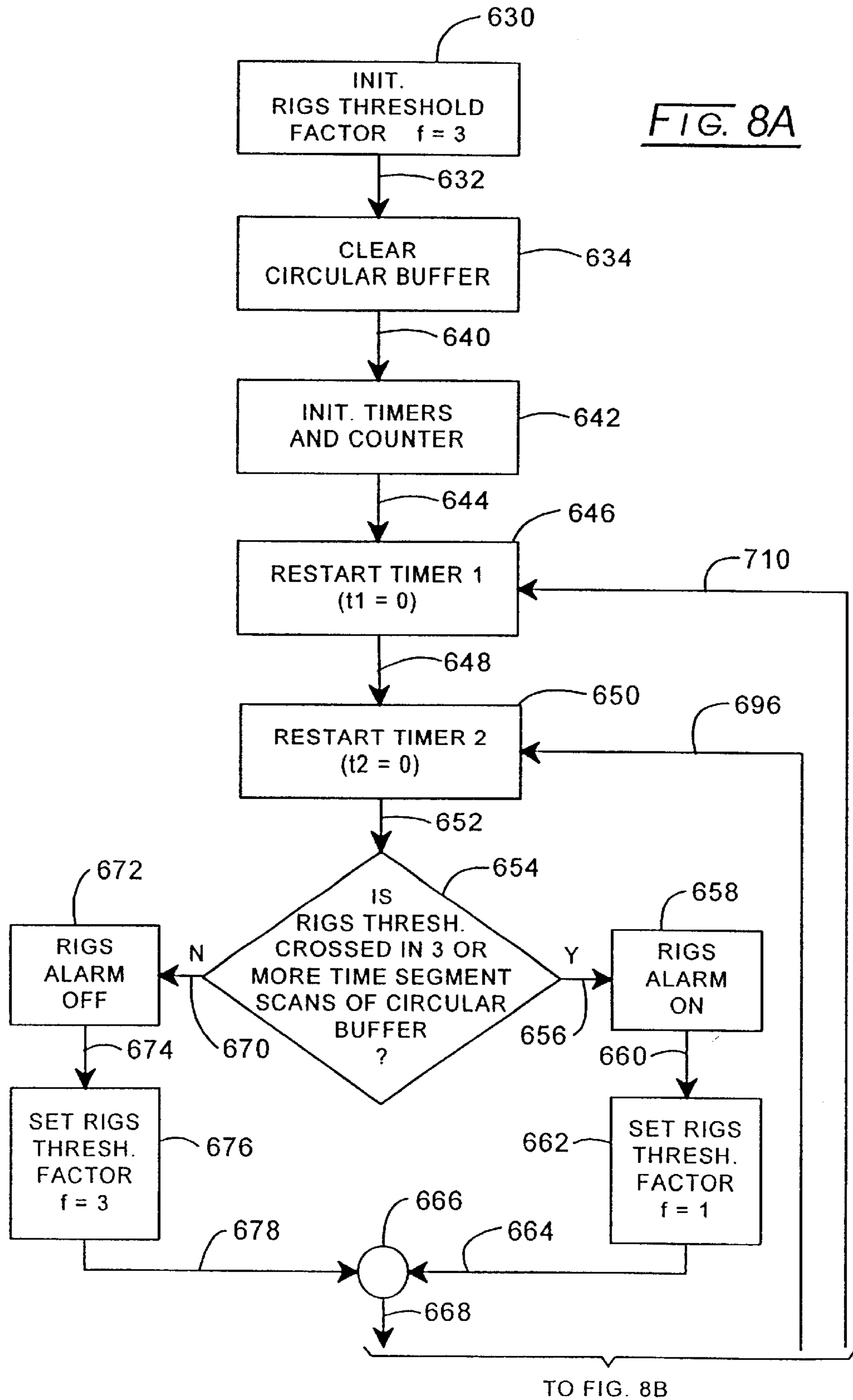
FIG. 5D

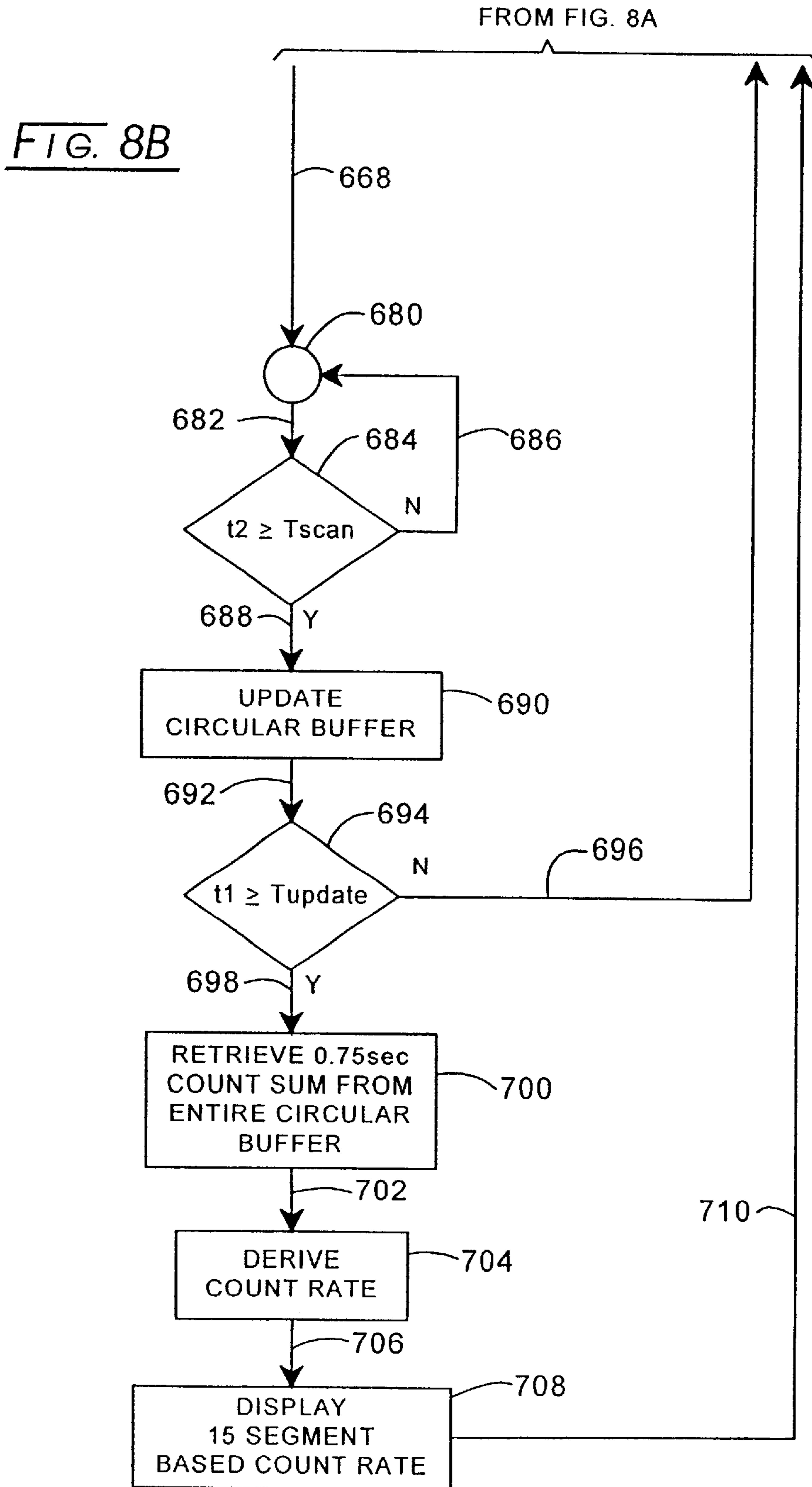
FIG. 6A











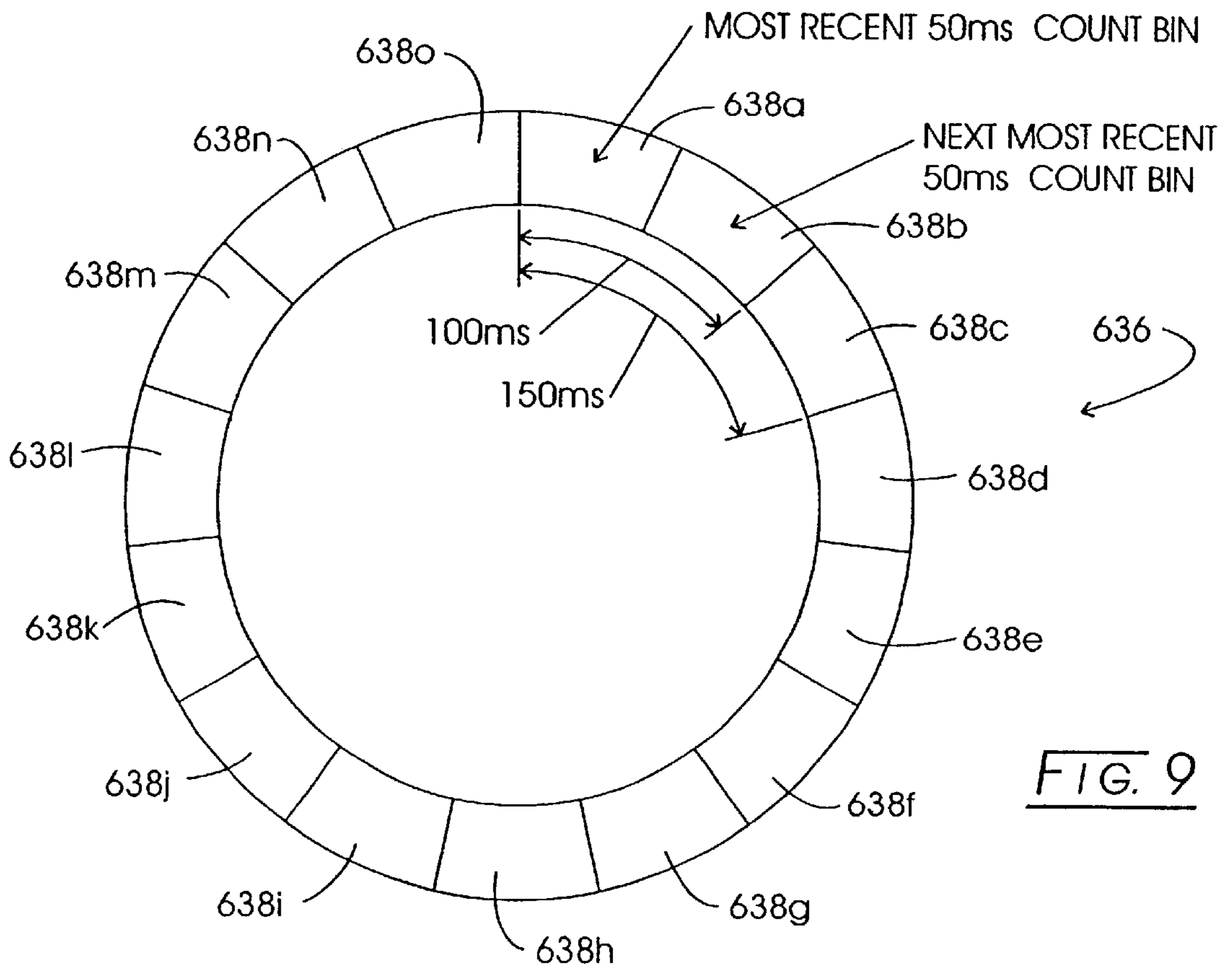


FIG. 9

## SCANNING SYSTEM AND METHOD FOR LOCATING SOURCES OF RADIATION EMISSION

### BACKGROUND OF THE INVENTION

Current and historical procedures for treatment of colon and rectal cancer generally have been based upon the natural history of tumor spread, and thence, upon operative and non-operative options available to the practitioner. Operative options generally have looked to the physical identification and surgical resection of tumor. A variety of techniques have been brought to bear in the art with the purpose of aiding the surgeon in detecting and localizing neoplastic tissue as part of this surgical procedure. ("Neoplastic tissue," for the present purposes, often is referred to as cancerous tissue, though malignant tumor and malignant tumor cells also are found in the terminology of the art. The term "neoplastic tissue" includes all of these.) A substantial amount of the effort which has been expended in seeking to aid the surgeon in the process of locating neoplastic tissue has been concerned with the utilization of radiolabeled antibody. For example, one technique includes the scintillation scanning of patients who have been injected with relatively high energy, e.g.  $^{131}\text{I}$  labeled antibodies. Such photoscanning scintigrams are difficult to interpret because of blood pool background radioactivity. Computer subtraction of radioactive blood pool agents and the use of two labeled antibodies (one specific for the tumor and one non-specific) have been attempted in an effort to enhance imaging. Nevertheless, such techniques have been found to provide little, if any, useful information to the surgeon, especially over and above the CAT scan, magnetic resonance imaging, and like traditional techniques. Typically, large tumor is readily located by the surgeon by visualization at the operating theater, and, in particular, through palpation, i.e. the feel of tumor as opposed to that of normal tissue. To achieve operative success, however, it is necessary for the surgeon to somehow locate "occult" tumor, i.e. tumor which cannot be found by the conventional surgical procedures of sight and feel. Failure to locate and remove such occult tumor generally will result in the continued growth of cancer in the patient, a condition often referred to as "recurrent" cancer. In general, conventional diagnostic techniques such as, for example, use of the classic gamma camera and the like, fail to find or locate occult tumor. As tumor sites become smaller, the radionuclide concentrations at a given site will tend to be lost, from an imaging standpoint, in the background where blood pool radiation necessarily is present in the patient.

In 1984, Martin, M. D., and Thurston, Ph.D., introduced a much improved method for locating, differentiating, and removing neoplasms. Such technique uses a radiolabeled antibody and a portable radiation detection probe which the surgeon may use intraoperatively in order to detect sites of radioactivity. Because of the proximity of the detection probe to the labeled antibody, the faint radiation emanating from occult sites becomes detectable, for example, in part because of the inherent application of the approximate inverse square law of radiation propagation. The procedure now is known as radioimmunoguided surgery (RIGS®) (RIGS being a registered trademark of Neoprobe Corporation of Dublin, Ohio). The RIGS system for surgery additionally is successful because of a recognition that tumor detection should be delayed until the blood pool background of the circulating radiolabeled antibody has had an opportunity to be cleared from the body. As a consequence, the photon emissions or radiation emitted at minute tumors,

compared to surrounding tissue, becomes detectable in view of the proximity of the probe device to it. Fortunately, the radiolabeled antibody is capable of remaining bound to or associated with neoplastic tissue for extended periods of time with the radio tag still bound thereto. Moreover, even though the accretion of radioactivity at the tumor site decreases over time, the blood pool background and surrounding tissue (relative to the tumor sites) decrease at a much greater rate so that the radioactive sites can be determined readily utilizing a hand-held probe positioned in close proximity with the tissue under investigation. The seminal patent concerned with the RIGS procedure is U.S. Pat. No. 4,782,840 by Martin and Thurston, entitled "Method for Locating, Differentiating, and Removing Neoplasms," issued November 8, 1988, and assigned in common herewith, the disclosure of which is expressly incorporated herein by reference.

The important advances achieved through radioimmunoguided-surgery have been reported. See in this regard, the following publications:

- (1) "Radioimmunoguided Surgery system Improves Survival for Patients with Recurrent Colorectal Cancer" Bertsch, et al., *Surgery* 1995; 118: 634-639.
- (2) "Radioimmunoguided Surgery in Primary Colorectal Carcinoma: An Intraoperative Prognostic Tool and Adjuvant to Traditional Staging," Arnold, et al., *American J. Surg.* 1995; 179:315-318.
- (3) "The Significance of Intraoperative Periportal Lymph Node Metastasis Identification in Patients with Colorectal Carcinoma," Schneebaum, et al., *Cancer* 1995; 75: 2809-2817.
- (4) "Identification of Occult Micrometastases in Pericolonic Lymph Nodes of Dukes' B Colorectal Cancer Patients Using Monoclonal Antibodies against Cytokeratin and CC49," Greenson, et al., *Cancer* 1994; 73: 563-569.
- (5) "Intraoperative Detection of Occult Colon Cancer Micrometastases Using  $^{125}\text{I}$ -Radiolabeled Monoclonal Antibody CC49," Cote, et al., *Cancer* 1996; 77: 613-620.

The radioimmunoguided surgical system instrumentation is comprised generally of two basic components, a hand-held probe, as described above, which is in electrical communication via a flexible cable with a control console. This control console is located within the operating room facility but out of the sterile field, while the hand-held probe and forward portions of its associated cable are located within that field. The hand-held radiation detecting probe is relatively small and performs in conjunction with a cadmium-zinc-telluride detector or crystal.

The hand-held probe and preamplification electronics mounted within it in support of the cadmium-zinc-telluride crystal have been the subject of extensive scientific development. Cadmium-zinc-telluride crystals are somewhat fragile and exhibit piezoelectric properties which, without rigorous accommodation, will produce deleterious noise phenomena and the like. Further, the crystal and its operative associated preamplification function are called upon to detect necessarily very faint radiation. In this regard, only a very small amount of radioactive locator will be associated with minute, occult tumor. Thus, radiation emission count rates measured with the RIGS system are relatively low. Research activity concerning the above operational criteria is reflected in the following U.S. Patents.

U.S. Pat. No. 4,801,803 by Denen, Thurston and Ramsey, entitled "Detector and Localizer for Low Energy Radiation Emissions," issued Jan. 31, 1989.



U.S. Pat. No. 4,893,013 by Denen, Thurston and Ramsey, entitled "Detector and Localizer for Low Energy Radiation Emissions," issued Jan. 9, 1990.

U.S. Pat. No. 5,070,878 by Denen, entitled "Detector and Localizer for Low Energy Radiation Emissions," issued Dec. 10, 1991.

U.S. Pat. No. 5,151,598 by Denen, entitled "Detector and Localizer for Low Energy Radiation Emissions," issued Sep. 29, 1992.

To derive data representing the presence or absence of occult tumor, a microprocessor-driven complex system of analysis continuously works to statistically evaluate validated counts or gamma strikes to aurally apprise the surgeon of the presence or absence of occult neoplastic tissue. One algorithm under which the noted evaluation takes place is described in U.S. Pat. No. 4,889,991 by Ramsey and Thurston, entitled "Gamma Radiation Detector with Enhanced Signal Treatment," issued Dec. 26, 1989.

The RIGS system, not only having demonstrated its value in locating occult neoplastic tissue, also substantially aids the surgeon in determining the proper staging of the patient in accordance with the extent and severity of the disease. Such staging aids in determining the appropriate post-surgical treatment of patients. In this regard, an effective staging technique utilizing the RIGS system has been described wherein an R Number is determined in accordance with the formula:

$$R \text{ Number} = (n_1 E_1)_1 + (n_2 \times E_2)_2 + (n_3 \times E_3)_3 + (n_4 \times E_4)_4$$

wherein each subscript 1-4 represents an anatomic zone, staging of the patient being based upon the R Number determination. See generally, U.S. Pat. No. 5,482,040 by Martin, Jr., entitled "Biostaging of Adenocarcinomas Utilizing Radiolabeled Tumor-Associated Glycoprotein Antibodies," issued Jan. 9, 1996.

The RIGS system has been introduced into the field of laparoscopic surgery. See in this regard U.S. Pat. No. 5,429,133 by Thurston, et al., entitled: "Radiation Responsive Laparoscopic Instrument" issued Jul. 4, 1995 and U.S. Pat. No. 5,383,456 by Arnold and Thurston, entitled: "Radiation-Based Laparoscopic Method For Determining Treatment Modality" issued Jan. 24, 1995.

Cadmium telluride-based crystals, when employed in conjunction with the RIGS system perform admirably. Advantageously, higher purity levels for the compound crystals are not mandated in order to generate highly acceptable count-based outputs within an energy region of interest. Such performance, typically, is evaluated in conjunction with a multi-channel analyzer (MCA) relating counts with energy levels of interest. Where a sharp photopeak at the energy level of interest occurs which, in turn, is well spaced from regions of an MCA curve representing electrical noise, Compton scattering or the like, then windowing or thresholding out of such noise is a straightforward procedure. Cadmium telluride-based crystals achieve this excellent performance, inter alia, because they are used in conjunction with the radionuclide  $^{125}\text{I}$  which exhibits relatively low gamma energy (27-35 Kev). By contrast, the commonly employed  $^{131}\text{I}$  exhibits gamma energy of 360 Kev. The cadmium-zinc-telluride crystals employed with the RIGS system are, for the purposes of the instant discussion, considered to be "thin," i.e. having a thickness, d, of 2 mm. With the RIGS system, upon the occurrence of a photon event, a generation of carrier pairs generally will occur in a manner wherein holes are trapped at the grounded front face of the crystal. From that position they are immediately

collected by the initial integration stage of a signal treatment system. The carrier electrons, traveling at a velocity which is about twelve times greater than the rate of hole migration, all move essentially the same distance, such that, even if they are trapped, they are trapped to the same degree, and the result is an excellently performing crystal detection system.

Over the recent past, practitioners have been desirous of utilizing instrumentation similar to the RIGS system in conjunction with higher energy radionuclides. In particular, a call has been made for a cadmium telluride-based hand-held probe device which is operable in conjunction with the use of the radionuclide Technetium 99-m. The latter radionuclide exhibits a gamma energy level of, for example, 140 Kev. That value is somewhat excessive for the cadmium-telluride crystal architecture employed with the RIGS system. However, utilization of a hand-held probe with higher energy nuclides for the purpose of lymph system tracking is achieving importance.

The involvement of the lymph system in tumor metastasis has been the subject of extensive investigation and is well established. Lymphatic systems are present as widely dispersed tissues, fluids, and cells concerned in a variety of interrelated functions of the mammalian body including the circulation and modification of tissue fluid formed in the capillary beds, and the removal by mononuclear phagocytes of cell debris and foreign matter. The lymphatic system is importantly involved in participation with the blood vascular system in developing the immune response of the lymphocytes and other cells. Lymph flows within the system as a consequence of a variety of perceived mechanisms of organ and tissue dynamics. For certain cancers, metastasis, occurring in consequence of lymph drainage, will result in an initial location or positioning of neoplastic cells at certain lymph nodes typically deemed "regional nodes" within a pertinent lymph drainage basin. Some cancers, for example, melanomas, have been observed to exhibit variability in lymphatic drainage patterns emanating from different portions of the body. Other cancers, such as those encountered in the breast, will evidence somewhat more predictable nodal involvement. In designing forms of cancer disease management, therefore, efforts are directed to the identification of affected lymph nodes. For melanomas, it has been a more recent practice to identify the pertinent drainage basin or regional nodes along with an evaluation of the extent of lymph involvement with micrometastasis. A pre-surgical step undertaken in about 20% of investigational procedures concerning melanomas looks to the carrying out of a gamma camera generated form of lymphoscintigraphy which gives the clinician a gross two-dimensionally limited image, generally showing the tumor site injection of sulfur colloid labeled with Technetium 99-m ( $^{99m}\text{Tc}$ ) and, spaced therefrom, a region of radioactivity at the pertinent regional lymph nodes. The latter information at least confirms the path of drainage and the location of the proper drainage basin. Regional nodes then are removed and submitted for pathology evaluation.

For cancers, such as breast cancer, the sites of lymph node involvement are commonly encountered at axillary, internal mammary, and supraclavicular lymph node regions. Of these, the axillary lymph node region is the principal site of regional metastasis from carcinoma of the breast, and approximately 40% of patients have evidence of spread to the axillary nodes. In early approaches to the disease, these axillary nodes were removed as a form of therapy. Presently, however, their positive involvement, or lack thereof, has become the subject of diagnostics, as opposed to therapy. In this regard, the combination of the presence and extent of

metastasis to the axilla represents the single most important prognostic factor for the management of patients with breast cancer. See generally "Cancer, Principles and Practice of Oncology," vol. 1, 4th ed., DeVita, Jr., et al., chapter 40, Harris, et al., J.P. Lippincott Co., Philadelphia, Pa. (1993).

The axilla is a triangular region bounded by the axillary vein superiorly, the *latissimus dorsi* laterally, and the serratus anterior medially. With more current diagnostic procedures, essentially all axillary nodes at the axilla assumed to represent the drainage basin are removed during surgery for analysis. In general, somewhere between 10 and 30 nodes will be removed in the course of dissection with, of course, the attendant risks. In this regard, these nodes are generally surrounded by investment or fatty tissue and visualization of them necessarily is limited. Such dissection will pose risks of cutting the long thoracic nerve, the thoracic-dorsal nerve, the nerve to the *pectoralis major* or the axillary vein. Morbidity may occur in some cases due to regional node removal, and patients are known to frequently discuss a numbing of the arm region following the procedure.

While this form of somewhat radical axillary lymph node dissection has been the conventional approach to determining nodal metastatic involvement, more recent data suggests that less radical axillary node evaluation procedures may generate equivalent information for staging and patient management, but with far more limited dissection and resultant trauma, as discussed below.

Patient management for staging purposes for the case of cutaneous melanoma is highly predicated upon determinations of lymph involvement. A number of factors are involved in the prognosis of the disease, including, *inter alia*, location, tumor thickness, level of invasion, growth patterns, and, of particular importance, the identification of regional node metastatic involvement. Generally, surgical excision of metastatic nodes within the drainage basin of a lesion has been considered the only effective treatment for cure or disease control. Some investigators have preferred to excise only clinically demonstrable metastatic nodes associated with the lesion, while others have chosen to excise the nodes even where they may appear normal because of the risk of the presence of occult (clinically undetectable) metastasis. A substantial dialog has been carried on by investigators as to whether or not elective lymph node dissection, or lymphadenectomy, is an appropriate therapy. Elective lymphadenectomy has the major advantage of treating a nodal metastasis at a relatively early stage in its natural history when the tumor burden is low. On the other hand, such an approach may subject patients to surgery which would otherwise have been unnecessary. In particular, where patients exhibit a clinical Stage I level of the disease, there will be no nodal metastasis present, and no benefit then can be realized from regional lymphadenectomy.

Morton, et al., undertook an investigation of a procedure designed to identify that lymph node nearest the site of a melanoma and within the pertinent lymph drainage basin. Such a node, being on the most direct drainage pathway will present the most likely site of early metastasis and is referred to as the "sentinel node." Thus, by carrying out only a limited dissection, specific to this node and performing pathologic analysis of it, staging can be achieved without at least initial resort to more radical lymphadenectomy. With the approach, once the drainage basin from a lesion is identified, for example, by lymphoscintigraphy, an intraoperative mapping of the cutaneous lymphatics with vital dye is carried out at the time of surgical removal of the primary lesion. The vital dye, for example of blue color, is injected

at the site of the lesion and tracked by blunt dissection until the sentinel node is reached. That node is now exclusively of blue color and readily identified. Thus, the sentinel draining lymph node of each primary melanoma is isolated and removed. By examining the sentinel nodes, for example by frozen section using routine hematoxylin-eosin histopathological techniques, as well as rapid immunohistochemical techniques, only those patients who have evidence of micrometastasis in the sentinel draining node are subject to subsequent lymphadenectomy. See generally, Morton D., Wen D-R, Wong J., et al. "Technical Details of Intraoperative Lymphatic Mapping for Early Stage Melanoma," Arch. Surg. 1992: 127:392-399; and R.F. Uren, et. al, "Lymphoscintigraphy in High-Risk Melanoma of the Trunk: Predicting Draining Node Groups, Defining Lymphatic Channels and Locating the Sentinel Node," J. Nucl Med 1993; 34:1435-1440.

The approach of Morton, et al., also has been undertaken to moderate the otherwise somewhat radical axillary lymph node dissection common in staging breast cancer. Through the utilization of the noted vital dyes, in conjunction with the lymph drainage system from primary breast tumor, less radical sentinel node based procedures may result in adequate axillary staging and regional control. With the procedure, in general, a vital blue dye is injected into the breast mass and surrounding breast parenchyma. Following a relatively short interval, a transverse incision is made just below the hair bearing region of the axilla. Blunt dissection is performed until a lymphatic tract or duct leading to a blue stained node is identified. The lymph duct, having a blue color, provides a guide path leading to the location of the most proximal lymph node and thus the sentinel node. This sentinel node is excised and evaluated. While the procedure calls for considerable surgical experience and talent associated with the delicate task of following the blue duct (a ruptured dye-carrying duct can be problematic), the ability to identify a tumor-free sentinel lymph node will enable the surgeon to accurately stage metastasis-free breast cancer patients without subjecting them to the risks of radical dissection. The approach may also improve histologic staging by enabling the pathologist to focus on fewer lymph nodes. See generally Guiliano, A. E.; Kirgan, B. M.; Guenther, J. M.; and Morton, D. L., "Lymphatic Mapping and Sentinel Lymphadenectomy for Breast Cancer," Annals of Surgery, vol. 220, no. 3: 391-401, 1994, J.B. Lippincott Company.

As a replacement for or an adjunct to the tracking of portions of the lymph system to locate a sentinel lymph node, practitioners have injected the noted sulfur colloid labeled with <sup>99m</sup>Tc technician at the site of the lesion. Then, employing a hand-held radiation detecting probe, migration of the injectate along the lymph ducts to the sentinel node is carried out. Thurston, et al, in U.S. Pat. No. 5,732,704 entitled "Radiation Based Method for Locating and Differentiating Sentinel Nodes," issued Mar. 31, 1998, describe an improved technique for thus tracking a lymph duct and for utilizing a thresholding procedure three-dimensionally finding a radiolabeled sentinel lymph node with a hand-held probe.

As the use of radionuclides in the course of diagnostics and management of disease has expanded significantly over the past two decades, a concomitant need has arisen for instrumentation exhibiting a flexibility of use. Higher levels of computing power now are called for along with a flexibility or adaptability of performance. This calls for software driven equipment with software restructuring capabilities so as to readily convert equipment to new procedures and

techniques which may employ a wide range of different radionuclides. Equipment improvements facilitating readout values and enhanced surgical data reporting are needed by practitioners both to ease the burden necessarily imposed within the surgical theatre and to evoke higher levels of measurement accuracy.

#### BRIEF SUMMARY OF THE INVENTION

The present invention is addressed to a system, apparatus and method for detecting and locating sources of radiation wherein improvement is achieved in locating subtle or very small concentrations of radiation. The approach has particular applicability to the RIGS system for locating neoplastic tissue using a radionuclide tagged locator.

Quality in performance is achieved by combining a relatively short, 50 ms, scan interval with a computation of threshold count rate values for each of the number of combinations of the short scan interval counts. This approach is implemented with a circular buffer memory. Improved scanned performance further is achieved with an approach wherein a statistically related threshold factor,  $f$ , is altered to a lower value following an initial detecting threshold crossing condition. Six combinations of memory segment counts are tested against correspondingly computed thresholds. Three of those combinations must exceed their computed threshold for the initial activation of an audible cue under the higher threshold factor condition. The same test is applied subsequently under the lower threshold factor condition to maintain that audible cue.

A running count rate value is derived from the entire segment count contents of the circular memory on an intermittent, for example, one-half second basis. The entire memory compilation of segment counts will amount to 0.75 seconds. Thus, the cumulative or running rate will represent a form of 0.75 second averaging at an enhanced update rate.

Other objects of the invention will, in part, be obvious and will, in part, appear hereinafter. The invention, accordingly, comprises the method, system and apparatus possessing the construction, combination of elements, arrangement of parts and steps which are exemplified in the following detailed description.

For a fuller understanding of the nature and objects of the invention, reference should be made to the following detailed description taken in connection with the accompanying drawings.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a perspective view of a system according to the invention including a console and associated hand-held probe;

FIG. 2 is a front view of the console shown in FIG. 1;

FIG. 3 is a perspective view looking into the internal side of a forward housing component of the console shown in FIG. 1;

FIG. 4 is a perspective view of the forward housing component of FIG. 3 with the inclusion of power supplies and circuit boards;

FIGS. 5A–5D combine as labeled thereon to provide a block diagram of the control system employed with the console shown in FIG. 1;

FIGS. 6A–6C combine as labeled thereon to provide a flow chart describing the main program utilized by a central processor control of the console shown in FIG. 1;

FIG. 7 is a graph illustrating the performance of a floating window form of ILM count evaluation;

FIGS. 8A–8B combine as labeled thereon to illustrate a scanning program according to the invention; and

FIG. 9 is a schematic illustration of a circular buffer memory employed with the program of FIGS. 8A and 8B.

#### DETAILED DESCRIPTION OF THE INVENTION

Referring to FIG. 1, the system of the invention is represented generally at **10**. System **10** performs in conjunction with a hand-held radiation detecting probe represented generally at **12**. Probes, as at **12**, are selected to perform in conjunction with any of a number of medical procedures and, thus, may assume a variety of configurations. Predominately for the present purposes, however, the probe **12** will perform in conjunction with radioimmunoguided surgery procedures (RIGS) wherein a cadmium telluride crystal, based detector performs in conjunction with a systemically injected locator which, for example, may be an antibody labeled with the radionuclide  $^{125}\text{I}$ . That procedure may utilize probes having a general structure as shown at **12** or probes intended for laparoscopic surveys or investigations. Another predominant use of the hand-held probes is involved with intraoperative lymphatic mapping (ILM). ILM procedures generally employ a higher energy radionuclide such as  $^{99m}\text{Tc}$  which is injected at the situs of a lesion, and the probes then are utilized to locate that node within a lymph drainage basin designated as a “sentinel” node. Probes as at **12**, may assume a variety of configurations. In this regard where cadmium telluride crystal detectors are employed, then different operational modes for these crystals are utilized based upon the radionuclide energy involved. In general, probes as at **12**, will incorporate a forward structure as at **14** containing a crystal mount for retaining a detector crystal such as cadmium telluride. The forward face of such crystal typically will be in very close proximity but spaced from a radiation transmissive window as at **16**. Extending rearwardly from the forward structure **14** is a hand-grippable handle portion **18** which may support signal treatment circuitry such as preamplifiers and the like. A pulsed output is generated from this preamplification function in response to photon events or interactions with the detector crystal, and such pulsed outputs are conveyed, typically, by a flexible cable or suitable transmission assembly as at **20** to a control assembly represented generally at **22**. In this regard, a connector **24** at the outward end of flexible cable **20** is connected in electrical association with the corresponding connector **26** of the assembly **22**.

Control assembly **22** is seen to be formed having a forward housing component **28** of generally rectangular peripheral design. Forward component **28** is joined with a rear housing component represented generally at **30**. This component **30** includes a rectangular forward support portion **32** which meets with the rearward edge of forward housing component **28**. Additionally, the rear housing component **30** includes a rearward support portion **34** having a somewhat triangular cross section and which is integrally molded with the forward support portion **32**. This provides for the support of the forward housing component **28** at a convenient, rearwardly tilted orientation as shown. Preferably, the amount of such tilt is about  $57^\circ$ . This angularity facilitates manual switch actuation and adjustment by the user as well as promotes the readability of a readout display. Inasmuch as the control assembly **22** is powered from a conventional A.C. line voltage source, a cord wrap fixture **36** is molded within the rearward support portion **34**. In general, the forward housing component **28** and rear housing component **30** are injection molded of an

ABS/Polycarbonate blend which is resistant to the solvents and disinfectants typically encountered in the medical field. It may be noted that a parting line or joint **38** is present at the juncture or union of forward housing component **28** and the rectangular forward support portion **32** of rear housing component **30**.

The forward face of the control assembly **22** is represented generally at **40** and is seen to support a relatively large readout main display window **42**. Window **42** is formed of a polycarbonate that will make a strong weld joint with the ABS/Polycarbonate forward housing component **28**. The view through the display window **42** is enhanced by an anti-glare coating, and an ultraviolet cured coating is employed with the window **42** to improve its scratch resistance. All front housing transparent components are ultrasonically welded in place to assure that liquids will not breach the enclosure. Between the window **42** and the forward housing component **28** is a graphics overlay which contains informational symbols and functions to provide organization to multi-segmented character forming light emitting diodes (LEDs) mounted just rearwardly of the forward face **40**, including window **42**. Such LEDs serve to provide a very bright and readily discerned visual readout perceived by the surgeon working at the somewhat remote sterile field of a surgical theatre.

The most predominately utilized manual control components are mounted at the forward face **40** of the control assembly **22**. In this regard, where switches are employed, they are formed of a silastic button style configuration, for example a material sold under the trade designation "San-toprene" marketed by Scientific Molding Corp., of Somerset, Wis. Looking to the switch assemblies, an on/off switch is provided at **44** at one side of the display window **42**. Adjacent the opposite side of display window **42** is a "target" switch **46**. When the momentary on target switch **46** is pressed and immediately released, a "target check" procedure representing a two second count by the probe **12** is carried out. Where the switch **46** is held on or actuated for at least one second, a "target count" procedure is carried out for an interval of six seconds. These latter count intervals are exclusive to the operation of system **10** in a RIGS mode. Next below the switch **46** is a background count switch **48**. Switch **48** is used in a RIGS mode of operation for the development of statistically significant thresholds, counting for background occurring utilizing probe **12** at a predetermined location during and just prior to surgery. Next below the background count switch **48** is a mute switch **50**. During some procedures, the practitioner will wish to avoid the audio output of the system with the exception of aural feedbacks for switch actuation. Accordingly, those former sounds may be muted by actuating switch **50** which will perform in all operational modes including RIGS and ILM. The level of audio output is controlled by a volume encoder shown as a knob **52**. Encoder **52** provides a coded input of from one to **128** positions such that control software can provide a broad variety of audio output volumes depending upon the mode employed with the system **10**.

Below the center of display window **42** is a mode selection switch **54**. Actuation of switch **54** alternately elects one of the two predominate operational modes of system **10**, i.e., a RIGS procedure, which will result in the illumination of an elongate rectangular output display at **56**. This RIGS mode of operation additionally is referred to as "binary pitch" operation. Alternate actuation of switch **54** will elect an ILM operational mode with the illumination of an elongate rectangular output display **58**. The latter mode of operation also is referred to as a "dynamic pitch" operation. For the latter

operational mode, in view of the high energy level and larger quantities of radionuclide material employed, count rate ranges may be elected by the operator. Accordingly, an array of range switches represented generally at **60** are mounted at the forward face **40**. The momentary push switches are shown at **61-64** and respectively correspond with ranges of 0-100 CPS, 0-1000 CPS, 0-10000 CPS, and 0-50000 CPS. With the election of a given range by actuation of one of the switches **61-64**, a corresponding range indicator, shown respectively at **66-69**, is illuminated. In general, each of the ranges will incorporate an initial threshold level below which no audible or visual cueing will occur. That range, for example, may be 2% of the maximum count value for the given range. The ranges also may be restricted by a background count initiated at switch **48**.

Referring to FIG. 2, the forward housing component **28** again is revealed. However, shown at the display window **42** are visual readouts which are generated in conjunction with the operation of system **10**. To facilitate the ease of operation of the system **10**, on a worldwide basis, icon imagery or graphical labels are employed, inter alia, in conjunction with the switches **46**, **48** and **50**. Colors also are used to indicate relationships between data items and to enhance understanding of the displays. Further, the visual indicators have the ability to be flashed or energized intermittently in order to draw attention to a given data or procedural item. The indicators also are operated in a manner to help differentiate between a period when the data item is being acquired by system **10** and the period when the acquired data then is being displayed. In this regard, a flashing indicator generally means that the associated data item is being updated as a result of an operator action.

Running count rate data is published at the window **42** with a large bright LED derived segmented character representation which is located generally horizontally from the target switch **46**. This numeric readout is shown at **80** in FIG. 2. During the operation of the system **10** when the target counts are not underway in consequence of the actuation of switch **46**, the count rate data published at **80** is updated each ½ second. However, where the practitioner actuates the target switch **46**, for example, in a RIGS mode of operation to derive a target check, then the numeric data at **80** disappears in favor of dashes and an icon assembly containing an icon **82** with the shape of an international target is intermittently energized or flashed for the two second collection period. This same flashing occurs in conjunction for example, with the six second target count data collection occurring during the RIGS mode of operation. Following the data collection interval, then the target count or target check count rate information is published utilizing the numeric output **80** and is sustained at the window **42** for the relatively short display interval, for example of five seconds. Following that display interval, then the conventional ½ second updated count rate data is published in conjunction with the readout indicia as at **80**. At the opposite side of the display window **42** there is provided a sixteen segment bar graph represented in general at **84** and having bottom and top (first and last) illuminated segments shown respectively at **86** and **87**. To appraise the practitioner of the amount of time remaining for the collection of data associated with the actuation of target switch **46**, the LED implemented sixteen segment bar graph **84** will "fill" or illuminate segment by segment from bottom segment **86** toward top segment **87** during the predetermined data collection intervals. Thus, the surgeon will be aware of how much additional time the probe **12** should be retained in count position. When the system is operated in an ILM mode, this same form of

information is provided, however, it is tempered or improved with respect to a number of data points collected representing an adequate degree of confidence. This follows, for example, in the ILM mode because of the relatively larger count rates involved, permitting a rapid development of confidence levels. Thus, with the exception of lower and upper bounds in data collection times, at higher count rates the segments of the bar graph **84** will fill for this ILM procedure on an expedited basis.

Actuation of the background switch **48** while system **10** is in a RIGS mode will cause the carrying out of a six second background count evaluation. During the progress of this background counting, a background icon assembly **90** represented as a dual ring is energized on an intermittent or flashing basis. While the six second counting ensues, the bar graph **84** will correspondingly "fill" from lower segment **86** to upper segment **87** in correspondence with that set six seconds. The background value will be published as numerical indicia as at **92** at the termination of the interval. With the completion of background computation, the system **10** will compute a ratio of background count rate to the currently measured count rate and publish it as at **98** along with a ratio indicia (**97**) intermediate icons **82** and **96** and indicia **80** and **92**. During the ILM mode, the bar graph **84** publishes count rates over the earlier noted default threshold or, when utilized, over a background count ratio, the segments of the bar graph **84** are energized from first to last in accordance with the difference between either threshold or background and the current level of count. Such display also reflects the range selected from the switch array **60**. The audio output of the system **10** when operating in the noted ILM mode, also provides a varying pitch or frequency output which is compressed between the lower threshold or background count and the upper frequency limit.

Actuating the mute switch **50** in the course of a procedure provides for the energization of a mute icon assembly represented at **94**. The icon **94** so displayed represents a sound wave pattern with a slash positioned across it. Also illuminated during the course of a procedure at one of six rectangular positions across the bottom of display window **42** is an illuminated indication of the type of radionuclide utilized. The ILM mode indicator, depicting  $^{99m}\text{Tc}$ , is shown in FIG. 2 at **96**. The system **10** defaults to this indicator upon actuation of switch **54** for one mode. Correspondingly, another actuation of mode switch **54** will illuminate a similar indicator at the opposite side of window **42** showing a  $^{125}\text{I}$  radionuclide utilization. Four other radionuclides may be selected with the system by actuation of a switch (not shown) mounted at the rear housing component **30** (FIG. 1). Radionuclides which may be elected are, for example:  $^{57}\text{Co}$ ,  $^{111}\text{In}$ ,  $^{18}\text{F}$  and  $^{131}\text{I}$ , and at such time as the system **10** is activated, but probe **12** is not connected properly or is inoperative, a probe defect icon as at **99** is energized at the lower left side of display window **42**.

The software driven control features of system **10** perform in conjunction with a standard bus architecture referred to as "PC/104." This standard bus approach is desirable in view of a small form factor (3.55 inch×3.25 inch) which reduces crowding within the control assembly **22** enclosure. Control architecture including a CPU board, an I/O board, a DSP board and a unique pulse detector module (PDM) are mounted to the PC/104 mother board or backplane and are located outwardly from but parallel therewith. The forwardly directed surface of this backplane functions, inter alia, to support the LED based circuits associated with display **42**, as well as the range displays **66–69** and the mode selector displays **56** and **58**. That face of the board also

cooperates with the manually actuated components of the switches at forward face **40**.

Looking to FIG. 3, the rearward side of forward housing component **28** is revealed as it appears before the positioning of the noted backplane and its associated and supported components. In FIG. 3, a tongue-in-groove form of edge connection as described in FIG. 1 at parting line **38** is revealed with the same numeration. To provide for EMI filtering, the entire interior surfaces of both the forward housing component **28** and rear housing component **30** are coated with an aluminum containing conductive material which is vacuum deposited. To preserve the integrity of the shield at the union between components **28** and **30** as at parting line **38**, the interior surface of forward housing component **28** supports a plurality of EMI gaskets **100a–100r** formed, for example, of beryllium-copper spring-like material. When the forward housing component **28** is mated with rear forward support portion **32** of rear housing **30**, the gaskets **100a–100r** complete the EMI security feature. Switches **46**, **48** and **50** are formed having silastic cup-shaped cover assemblies which extend through openings within the forward face **40**. As they extend through that forward face, the outwardly flared inward edges of these switch covers are compressibly retained against the rear surface **102** of forward housing component **28**. To secure them in this compressed arrangement, a metal switch-plate **104** is secured against them using machine screws. In similar fashion, cup-shaped silastic switch cover assemblies **54a** and **61a–64a** are retained at the back surface **102** by a metal switch-plate **106**. In general, when the practitioner depresses one of the elastomeric cup-shaped switch cover assemblies, contact is made with corresponding conductive switching elements which are supported upon the forward face of the noted backplane. The minimization of discrete wiring thus achieved is a substantial advantage in fabrication of the control apparatus **22**.

To avoid cross talk or light scatter, for the most part, the LED illuminated display features including icons, indicators and numerical indicia as well as bar graph **84** are formed as assemblies with baffles isolating the light emitting components. In this regard, the circular icons including target icon **82**, the ratio icon (**97**) background icon **96** and mute icon **94** are retained within respective light restricting cylindrical baffle channels or wells **108–111**. In similar fashion, the numerical indicia representing general count rate as at **80** and the ratio valuation **98** just below it are retained within a rectangularly shaped light restricting channel **114**. Adjacent to light restricting channel or baffle **114** is another vertically oriented rectangular light restricting channel **116** at which the multi-segment bar graph **84** is located. Adjacent to channel **116** is another light restricting cylindrical baffle or well **118** which surrounds an LED array functioning to illuminate icon **99** representing that probe **12** is inoperative. Below the light restricting channel **114** and baffle **118** is another rectangular light restricting channel **120** which is employed with background count rate numerical indicia published by LED formations mounted upon the noted backplane. Next below the channel **120** is a horizontal sequence of six light restricting channels or baffles of generally square configuration which function to confine light extending to a display showing the earlier noted radionuclide identifications including, for example, that for  $^{99m}\text{Tc}$  shown at **96** in FIG. 2. This array is represented generally at **122**. Below the array of light restrictors **122** are two elongate rectangular light baffle channels **124** and **126** which surround LED illuminator arrays providing the mode indicator illumination described at **58** and **56** in FIG. 2. Next

extending below the channel **124** is a sequence of four rectangular channels **128–131** which baffle and confine light from light emitting diode arrays serving to illuminate the respective range indicators **66–69** described in FIG. 2. Access for the volume encoder knob **52** as seen in FIG. 2 is provided through an opening **134** which, as with all the above described components, cooperates with the backplane. Additionally shown on the drawing are a plurality of standoffs, some of which are identified at **136**, which are employed for purposes of securing the backplane or mother board to this forward housing component **28**.

Turning to FIG. 4, the forward housing component **28** again is shown but with the installation of the noted backplane with standard PC/104 bus and associated backplane mounted components. In the figure, the backplane is represented in general at **150** and is seen to have a thin rectangular structural aspect dimensioned to be positioned against the rearward structure of component **28** as described in connection with FIG. 3. Mounted upon the rearward face of backplane **150** is a generally horizontally disposed open-framed 12 volt power supply represented generally at **152**, and vertically oriented in adjacency therewith is a 5 volt open-framed power supply represented generally at **154**. Each of these power supplies are electrically connected with an a.c. utility input introduced from the rear housing component **30** (FIG. 1). That a.c. input is directed via a cable seen in FIG. 4 at **156** which extends through an a.c. line filter **158** and thence, as represented at **160** to power supplies **152** and **154**. Additionally coupled with this input and power supply circuit is the power, on/off switch **44** terminal at **162** which is supported on the backplane **150**.

Positioned in parallel stacked relationship and in electrical communication with the bus architecture of the backplane **150** are four rectangularly-shaped circuit boards. As before, by being associated with this standardized bus structure, substantial numbers of lead connections are eliminated, and the more ideal data transfer interconnections of a bus system are realized. Further, such structuring provides independent upgradability of each circuit board under the PC/104 standards criteria. Power converter grounds are provided from the rear of the assembly **22** from flexible cables as seen at **164** and **166**, while in similar fashion, probe **12** ground input is provided from the rearward component **30** of assembly **22** by a flexible cable connection as represented at **168**. This connection **168** extends to a probe dedicated terminal **170** which, in turn, is electrically associated with the input connector **26** (FIG. 1). Terminal **170** is seen in electrical connection with a printed circuit board **172** upon which is formed a signal treatment circuit. In this regard, the board is generally referred to as a pulse detector module board (PDM). Mounted to the rearward face of backplane **150** by standoffs, two of which are revealed at **174** and **175** and multiple pin connectors (not shown) the signal treatment carried out at the board **172** is one treating the pulse output from a preamplification stage contained within the probe **12** itself. Connected within the bus architecture and parallel adjacency with PDM board **172** is a printed circuit board **178**. As before, mechanical connection is made utilizing standoffs, two of which are seen at **180** and **181** and multiple pin connectors. Board **178** supports a digital signal processor circuit (DSP). The DSP component utilized with board **178** is a type TMS **320** series by Texas Instruments, Inc. of Dallas, Tex., and the board employing that DSP is a Starburst type **104C31** marketed by Nova, Inc., of Cincinnati, Ohio. On the opposite side of the 5 volt power supply **154**, there is provided an input/output circuit board **182** which provides a **48** line I/O function performing in conjunction

with the standardized bus architecture. The board **182** may be provided, for example, as a part number EMM-DIO-PO, by Diamond Systems, Inc., of Polo Alto, Calif. Mounted over and in parallel adjacency with the board **182** is a central processing unit board **184** (CPU). The CPU board **184** may be provided, for example, as a model 4 DXi marketed by Ampro, Inc., of San Jose, Calif. The CPU function at board **184** is a 133 MHz 486DX based PC/104 board with onboard programming of flash memory, floppy/IDE interface, serial ports, parallel port and serial boot loader capability. Software and onboard programming capabilities enables the software of system **10** to be upgraded without removing board **184** from the control assembly **22**. Cables associated with the CPU function at board **184** are seen at **186** and **188** while I/O cable is seen at **190**. Not shown in the figure but mounted for access at the rear housing component **30** is an auxiliary board carrying a manually actuatable switch for selecting any of the earlier six noted radionuclide mode setups. Additionally, a data (serial) port is provided which is electrically associated with the central processor control at board **184**. Further included but not shown in the drawing is a cooling fan mounted at rear housing component **30**. A connector is shown at **192** mounted upon backplane **150**. It may be used in conjunction with the noted auxiliary board.

FIGS. 5A–5D are block diagrammatic representation of the control system. These FIGS. 5A–5D should be considered in an orientation established by the labeling thereon. Referring to FIG. 5A, connector **26** is represented in general as looking to four components of the interface of control apparatus **22** with the probe **12**. In this regard, as represented at line **200**, a data signal present as a pulsed output will be carried by a line represented at **200**. From the control circuitry, a voltage bias is provided at line **201** for the operation of the detector component of the probe **12**. Similarly, ground as represented at line **202** is carried to the probe **12** detector component and, as represented at line **203**, circuit power, for example at +12 volts, is supplied to the probe **12**. Lines **200–203** are shown in operative association with a probe interface circuit function represented at block **204**. The pulsed output as provided at line **200** generally will exhibit a narrowness which, in terms of time, will be of two to seven microsecond duration at 10% of its height. From the interface function **204**, the pulse signal or pulse train is introduced, as represented at arrow **206**, to an EMI filter network represented at **208**. Stage **208** functions to remove very high frequency EMI noise and has no operational effect upon the pulsed output. From the filtering function **208**, as represented at arrow **210** and block **212**, the pulsed output is buffered. In general, the buffer stage **212** is implemented as a unity gain operational amplifier. The thus buffered signal, as represented at arrow **214**, then is submitted to a baseline restoration network represented at block **216**. In general, the function at block **216** is one incorporating an a.c. coupling capacitor. At very high pulse rates, without baseline correction, the resultant pulse train tends to degrade, falling below the lower threshold of a window circuit which is later encountered. To correct for this phenomenon, a time-dependent base line restoration network is provided which derives a soft clamp retaining the output of the coupling capacitor at, for example, ground in the absence of a pulse. This avoids the noted downward drift of the pulse train. The advantage of this form of baseline restoration resides in its immunity to any distortion of pulse height. Thus, probes of different operational pulse widths can be employed with the system. From the baseline restoration at block **216**, as represented at arrow **218** and block **220**, the signal then is amplified. The amplification stage represented at block **220**

is one, for example, providing a gain of 2.5. The resultant amplified signal then is present at arrow 222. That output is tapped as represented at arrow 224 to provide the noted time dependent input to the baseline restoration network 216.

Looking additionally to FIG. 5B, arrow 222 reappears as it directs the amplified probe signal to a validation network including upper limit and lower threshold energy comparators as represented at block 226. The network 226 identifies those pulses which are above a lower threshold reference which, for convenience, is provided at ground and which exceed a reference level representing an upper limit. The resulting data then is presented, as represented at arrow 228, to an energy and pulse width discriminator function represented at block 230. In general, the function 230 is implemented with a programmable logic device (PLD). This logic device validates the pulses which are below the upper limit and above the lower threshold of the window function represented at block 226. Additionally, the function at block 230 times the pulse identification at the lower threshold of the window comparator function at block 226 to determine pulse width. Experience with the system 10 has shown that valid pulses will exhibit a pulse width at that lower threshold of less than about 12 microseconds. Lengthier pulse widths statistically will represent noise. Thus, a logical ANDing activity occurs at the function 230 requiring pulse validation with respect to the windowing function represented at block 226 and with respect to pulse width as evaluated from the lower threshold comparator of the windowing network. The PLD device implementing function 230 performs under the supervision of a central processor control or central processing unit (CPU) as represented at block 232 and arrow 234.

Upon being validated, a pulsed output then is transferred to a digital signal processing activity (DSP) as represented by arrow 236 and block 238. This DSP network has been described in conjunction with DSP circuit board 178 in FIG. 4. The DSP function 238 is slaved to or controlled by the central processor control 232 as represented at arrow 240 and provides signal information thereto as represented at arrow 242. Data transfer with respect to the PC/104 bus architecture between the DSP function at block 238 and the central processing function at block 232 is represented by the bus arrow 244. In general, the DSP function 238 develops count rate data in accordance with a variety of algorithms which additionally determine the statistical significance of count rates with respect to background count rate and the generation of count rate data which is displayed at display window 42.

As represented by arrow 246 and block 248, the central processor function 232 also develops an analog reference voltage level which is employed to provide the reference level for the upper limit and lower threshold comparators at the window function represented at block 226. A digital-to-analog function, which is made available at the DSP board function represented at block 238, is utilized for this purpose. However, in the interest of clarity, the function is shown as a separate block. By providing a control over the analog reference level from the central processor and DSP 238, that processor can react to the selection of a particular radionuclide by the user and automatically apply the proper window references. In this regard, the analog output from the function represented at block 248 is directed as represented at arrow 250 to a reference ranging network represented at block 252. The ranging function at block 252 asserts a precision with respect to the applied analog reference level by performance with a precision reference voltage developed at the PDM circuit board 172 described in conjunction with FIG. 4. The appropriately perfected references

then are supplied to the upper and lower energy window comparators as represented by arrow 254.

The central processor control function 232 also receives volume data selected by user manipulation of knob 52 (FIG. 1) from an input/output circuit 302 via the bus architecture. The encoding function is represented in FIG. 5C at block 256, while bus-related communication is represented at bus arrow 258. Serial port communication also is provided at the central processor control function 232 as represented at block 260 and by-directional arrow 262. Such communication with the central processor control function 232 permits the reprogramming of system 10 to accommodate future requirements. Control, as represented at arrow 264 also is provided from the central processor control function 232 to a bias selector network represented at block 266 in FIG. 5A. The selector network 266 responds to a digital input to effect the application of a particular bias voltage level at line 201 for presentation to a particular probe as at 12. In general, that bias level will be selected in response to the election by the user of a particular radionuclide. In this regard, it may be recalled that a radionuclide selector switch is provided with the control assembly 22 at its rear housing component 30, and selection of the two most predominating radionuclides is made at switch 54 located at the forward face 40 of assembly 22. These bias levels may be the same for given or selected ones of the radionuclides or may be different depending upon the probe and associated detector architecture. To provide an initial bias voltage supply, an unregulated relatively higher voltage supply as provided at the PDM circuit board 172 is represented in FIG. 5A at block 268. As represented at arrow 270, that bias voltage is delivered to a comparator and current limit network represented at block 272. The comparator network 272 responds to a selection signal from the network represented at block 266 as represented at arrow 274 to develop a predetermined bias level for delivery to the probe interface function represented at block 204 as, in turn, represented at arrow 276.

Referring to FIGS. 5B and 5C, the PC/104 bus architecture is represented at bus arrows 278 and 244 as being in control-asserting communication with a variety of switching and user perception associated outputs. As represented at block 280, an audio network is provided which may be a type ES1688 marketed by ESS Technology, Inc. That highly integrated device interfaces directly with the bus architecture of system 10. The network function represented at block 280 includes a speaker and amplifier, the speaker being mounted at the bottom of the rear housing component 30. FIG. 5C identifies the switching functions and probe detection features of the system 10, as they perform in conjunction with the bus 278. In this regard, the bus arrow 278 is seen to branch at 282 for communication with the switches described in connection with FIG. 1. For instance, the range switches 61-64 are associated with the bus; mode switch 54 also is so associated with the bus; target count switch 46 is coupled into the bus architecture; background count switch 48 also is so connected and mute switch 50 is associated with bus 282. These switch functions are represented at block 284 and they further are associated within the bus architecture, as represented at bus component arrow 286, with a switch debounce network represented block 288. The radionuclide select switching function shown at block 290 mounted at the rear housing component 30 also is functionally associated with the bus architecture as represented at 282. Through that bus architecture shown as at bus component 291 the bus system provides an input through debounce network 288. System 10 also provides a signal output in the event that probe 12 is inoperative, for example, not being

properly connected with the control assembly 22. That probe detect function is represented at block 322 in FIG. 5A in association with arrows 214 and 320. A probe signal is delivered, as represented by arrow 324 to PLD network 230 (FIG. 5B) and thence into the bus architecture. The probe detect signal associated with bus component 282 is shown to extend through bus component 294 to the debounce network 288. Finally, the probe 12 may be configured having one or more switches mounted upon its handle. Typically, those switches will emulate target switch 46 and/or background switch 48. Such a switching feature is represented at block 296 in association with the bus architecture 282 and through bus component 298 with the debounce network 288. Debounce network 288 is associated through the bus architecture as represented at bus arrows 300 and 278 with input/output (I/O) network 302. Network 302 additionally is seen associated with the bus architecture bus component 278. The I/O network 302 is mounted upon the I/O board 182 described in connection with FIG. 4.

Looking to FIG. 5D, the bus architecture component 278 is seen to continue its association with a variety of display features. These displays are illuminated with LED arrays under control ultimately of the central processor control function represented at block 232. One count display, such as that represented at 92 in FIG. 2 associated with the background count, is represented in FIG. 5D at block 306. Positioned upwardly from that display is a ratio value display which is represented at block 308. In general, the ratio display is provided in conjunction with the target count development which, it may be recalled, requires a six second count reading when system 10 is operating under the RIGS mode. No such ratio display is provided during the shorter duration target check associated with switch 46. The bar graph and radionuclide display is represented at block 310 to facilitate user perception, the lowermost and uppermost segments of the 16 segment bar code display are illuminated in a different color than the other segments, for example, they may be illuminated in an amber color while the intermediate segments are illuminated in a green coloration. A "cumulative" count value display is that associated with the output described at 80 in FIG. 2 and is represented herein at block 312. A mode display is represented at block 314. That mode display is one of those visually perceptible outputs at 56 or 58 as shown in FIG. 2. The icon displays including icons representing target count, ratio, background count, mute and probe detect are represented at block 316. Finally, a range display as associated with perceptible display outputs 66-69 is represented at block 318. In general, all of these LED arrays are supported from the forward surface of the backplane or mother board 150 (FIG. 4).

Referring to FIGS. 6A-6C, a flow chart illustrating the main program executed by central processor control 232 as it performs in conjunction with DSP processing function 238 is revealed. The program commences as represented at block 330 with the carrying out of power up. In general, this occurs with the actuation of power switch 44. Then, as represented at line 332 and block 334 initialization procedures are carried out. For these procedures, default values are acquired. If the probe detect function 322 indicates a non-connected probe 12, then 99 is illuminated at display window 42. The program then continues as represented at line 336 and block 338 to default to the last operational mode utilized. In this regard, the two modes concerned at this juncture are the ILM mode and the RIGS mode. For the present flow chart, only those modes are considered. The program then continues as represented at line 340 and block 342 to enter the mode elected. Should the user have changed

modes by actuation of switch 54, then that election will be present at this juncture in the program. For either mode, probe 12 is "scanned" along a region of interest. The term is intended to encompass all probe movement and stationary positioning occurring during a collection of photon event data. For the instant demonstration, assuming a RIGS mode has been elected, then the program proceeds as represented at line 344. This RIGS mode also is referred to as a "binary pitch" mode of operation. The RIGS mode of operation commences as represented at block 346 with a default selection of the radionuclide  $^{125}\text{I}$ , and the computer selects the reference values for the upper limit and lower threshold of the energy window function 226 accordingly. Continuing as represented at line 348 and block 350, the program then elects an appropriate bias for the selected radionuclide, in this case  $^{125}\text{I}$ . This is done by submitting information to the bias selector network 266. Then, as represented at line 352 and block 354, a background default value of seven counts per second is acquired. This background count generally will be altered by the practitioner with the actuation of the background count switch or button 48. Following the election of the default background value, as represented at line 356 and block 358, the RIGS scanning algorithm is activated. This algorithm is executed at the DSP processing function 238. In general, that algorithm utilizes a circular buffer form of temporary memory which is employed to collect validated photon event pulses in 50 millisecond time segment intervals. A statistically significant threshold valuation is computed with respect to each of predetermined combinations of those memory segments and where computed count rates exceed the computed threshold values in a predetermined number, then an aurally perceptible output is generated to apprise the surgeon that the probe 12 window 16 is adjacent tissue having a high probability of tumor involvement. After an initial threshold passage at a first statistical evaluation involving three standard deviations, the algorithm reverts to evaluations at a lowered standard deviation value. When the threshold is not met, on predetermined numbers of occasions, then the aural cueing is terminated and the higher statistical valuation is reasserted. The algorithm further retrieves count data from the circular buffer memory on a half second interval basis to publish a "cumulative" count rate as earlier described at 80 in connection with FIG. 2. The program then continues as represented at line 360 which line reappears in FIG. 6B. Looking to that figure, line 360 is seen directed to the decision block 562 wherein a query is made as to whether the background button or switch 48 has been actuated. In the event that it has, then as represented at line 364 and block 366, the background icon, as described at 96 in FIG. 2, is caused to commence to flash or be energized intermittently. Then, as represented at line 368 and block 370, the program calls the RIGS background program which carries out a count evaluation for a fixed interval of six seconds and, as that six seconds occurs, the bar graph 84 is proportionately filled from its lower segment 86 to its upper segment 87. This gives the surgeon a visual cue as to where in the background evaluation process the system 10 is. The program then continues as represented at line 372 and block 374 to carry out a displaying of the background count rate value at the location shown at 92 in FIG. 2 for a limited interval of five seconds. During the flashing of the background icon, the background count rate location as at 92 provides a dashed display. The program then continues, as represented at line 376 and block 378, to end the background icon flashing and, as represented at lines 380 and 382, to continue the program. Line 382 represents a program path followed additionally



where the inquiry posed at block 362 results in a negative determination. The program then continues to the query posed at block 384 wherein a determination is made as to whether the target switch or button 46 has been depressed and immediately released to cause commencement of a target check count evaluation. This target check evaluation calls for the collection of count data at a given location for a shorter interval of two seconds. In the event that the target check button condition is at hand, then as represented at line 386 and block 388, the target icon as described at 82 in FIG. 2 is caused to be energized intermittently, i.e. to flash. Then, as represented at line 390 and block 392 the RIGS target check program is called which, as noted, carries out a two second count evaluation. During this two second count evaluation, the bar graph 84 segments are filled from first to last, i.e., from segment 86 to segment 87. This, as before, provides the surgeon with a visual cue as to the status of this procedure. The program then continues as represented at line 394 and block 396 to provide for the display of the count rate developed from the target check procedure at location 80 in window 42. This display is only for a limited interval of five seconds. During the two second interval of collecting data, dashes are displayed at location 80. The program then continues, as represented at line 398 and block 400, wherein the icon flashing is terminated at the end of the five second display. As before, the program then continues as represented at lines 402 and 404. Line 404 additionally represents a continuation of the program where the query posed at block 384 results in a negative determination. Line 404 is seen to extend to block 406. At block 406 a query is posed as to whether a target count button actuation at switch 46 has been carried out. This occurs when the operator holds button 46 down for a one second interval. In the event of a negative determination, the program continues as represented at line 408. Where an affirmative determination is made with respect to the query at block 406, then, as represented at line 410 and block 412, the target icon as described at 82 in FIG. 2 is intermittently energized or caused to flash. Then, as represented at line 414 and block 416, the RIGS target count program is called to carry out a six second target count. During this six seconds, the segments of the bar graph 84 are illuminated from first to last or filled so as to apprise the surgeon as to the progress of this procedure. The program then continues as represented at line 418 and block 420 to cause a ratio icon as described at 78 in FIG. 2 to flash. Then, as represented at line 422 and block 424, the target count rate is displayed at location 80 as described in FIG. 2. Additionally, the ratio of the target count to the current background count is computed and displayed at location 76 at display window 42. These displays of target count and ratio values are transitory, being limited to an interval of 5 seconds. The program then continues as represented at line 426 and block 428 wherein at the termination of the five second display interval, the energization of the two pertinent icons is terminated. The program then continues as represented at lines 430 and 408. Line 408 is seen directed to the query posed at block 432 wherein a determination is made as to whether the mute button 48 has been pressed. In the event that it has not, then the program continues as represented at line 434. In the event of an affirmative determination with respect to the query posed at block 432, then the program continues as represented at line 436 and block 438. If the mute condition is active, then a mute icon described at 94 in FIG. 2 is energized intermittently or flashed. The program then continues as represented at line 440 and block 442 wherein the RIGS alarm mute function is toggled. In this regard, an aural feedback representing the mere pushing

of a switch button remains active in the system. However, all RIGS aural cueing is suppressed. The program then continues as represented at lines 444 and 434. Line 434 is seen directed to the query posed at block 446 wherein a determination is made as to whether the mode selection switch or button 54 has been pressed. In the event that it has, then, as represented at line 448 and block 450, the mode of system 10 is altered to an ILM mode and, as represented at line 452 and block 454, the ILM mode display 58 is illuminated. As represented at line 456 which continues into FIG. 6A the program loops to line 340 to commence an ILM mode of performance. In the event of a negative determination with respect to the query posed at block 446, then as represented at line 458 the program loops to line 360 to evaluate which actuation on the part of the operator.

Returning to FIG. 6A, where the program enters into an ILM or "dynamic pitch" mode of operation, as discussed above in connection with block 342, then as represented at line 460 and block 462, the radionuclide  $^{99m}\text{Tc}$  is elected and the program selects the appropriate reference levels for the upper limit and lower threshold energy windowing function 226. The program then continues, as represented at line 464 and block 466, to select the appropriate bias at the bias selector network 266 for the radionuclide at hand. Then, as represented at line 468 and block 470 default is made to an initial range of 10 to 1000 counts per second. The program then continues as represented at line 472 and block 474 to activate the ILM scanning algorithm, which algorithm is performed at the DSP processing function 238. In general, this algorithm employs a floating window form of analysis in conjunction with temporary memory implemented as a circular buffer memory. The floating memory approach provides a stability of both sound and visual output at the bar graph 84. Looking momentarily at FIG. 7, the floating memory approach is illustrated. In the figure, time in milliseconds is plotted against counts in cycles per second for a probe scan which transverses over a region of higher radiation value. The random counts,  $c$ , are represented by the dashed curve which is labeled with that variable. Note that the rate increases toward the middle of the plot and decreases at either end. A floating window is continuously computed on a timed basis and is seen to have an upper edge labeled UT and a lower edge which is labeled LT. From a computed upper edge UT, a reported mean is calculated and is shown as a solid line in the figure labeled RM. It is this reported mean, RM, which is utilized to generate a sound of varying pitch which elevates as the count rate increases. To accommodate for practitioners who are tone deaf, the frequency excursions are developed from one discrete pitch step to the next. In general, the pitch varies from 300 Hz to 1200 Hz. The same reported mean, RM, is used to drive the bar graph 84. It may be observed that the vertical width of the window defined between UT and LT in FIG. 7 varies in correspondence with the count rate level.

Returning to FIG. 6C, line 476 reappears leading to the query posed at block 478 determining whether the background button or switch 48 has been depressed. In the event that it has not, then the program continues as represented at line 480. In the event of an affirmative determination, as represented at line 482 and block 484, the background count icon 96 is intermittently energized or flashed and, as represented at line 486 and block 488, the ILM background routine is called. Further, bar graph 84 is energized in accordance with the amount of time required to achieve a background count. In order to expedite the interval for counting, the background count is developed from a predetermined number of count data points representing a corre-

sponding confidence level. Thus, where a higher count frequency is witnessed, the background count will be achieved in a relatively shorter interval of time, for example, less than a maximum interval of six seconds. Bar graph **84** will fill by sequentially energizing the LED segments thereof from **86** to **87** in a predicted time interval. However, the interval for filling the bar chart and developing background count is bounded by a minimum interval of two seconds and a maximum interval of six seconds. The program then continues as represented at line **490** and block **492** whereupon the developed background count is displayed at the character location **92** shown in FIG. 2. That display is present for the limited time interval of five seconds. At the termination of five seconds, as represented at line **494** and block **496**, the flashing of the background icon **96** is terminated and, as represented at lines **498** and **480**, the program continues.

In general, the cumulative ILM count rate is published at display location **80**. That count rate is developed from circular memory and is updated each one half second.

Line **480** is seen to be directed to the query posed at block **500** where a determination is made as to whether the target count button **46** has been depressed. It may be recalled that this actuation is one requiring the operator to hold button **46** down for one second. In the event of a negative determination, the program continues as represented at line **502**. In the event of an affirmative determination at block **500**, then as represented by line **504** and block **506**, the target icon **82** is intermittently energized or flashed and, as represented at line **508** and block **510** the ILM target count routine is called. Further, the bar graph **84** is filled utilizing the bounded predictive technique described in connection with block **492**. When the target count has been developed, then as represented at line **512** and block **514**, the target count is displayed at location **80** as seen in FIG. 2 for the finite interval limited to five seconds. The program then continues as represented at line **516** and block **518** to terminate the flashing icon **82** at the termination of the noted five seconds. The program then continues as represented at lines **520** and **502**. The program next proceeds to determine whether the mute button **50** has been pressed as represented at block **522**. In the event the mute button **50** has not been actuated, then the program continues as represented at line **524**. However, where the button has been pressed, then as represented at line **526** and block **528** the mute icon **94** is energized intermittently or flashed and the program continues, as represented at line **530** and block **532**, wherein the dynamic pitch count output for the ILM program is turned off. However, an aural feedback "beep" is maintained for any switch actuation. The program then continues as represented at lines **534** and **524**.

The program next proceeds to the query posed at block **536** wherein a determination as to whether any of the buttons or switches of the range switch array **60** have been pushed or actuated. In the event they have not, then the program continues as represented at line **538**. In the presence of an affirmative to that query, determination then as represented at line **540** and block **542** the dynamic pitch or sound output for the ILM program is altered to provide full scale output for the range selected. This same change is made with respect to the operation of bar graph **84**. This alteration also accommodates for any initial threshold value and background value. In particular, typically a 2% threshold is invoked for each of the ranges represented at the switch array **60**. Next, as represented at line **544** and block **546**, the pertinent range display is illuminated. These displays are shown in FIG. 2 at **66–69**. The program then continues, as

represented at lines **548** and **538**, to the query posed at block **550** wherein a determination is made as to whether the mode switch or button **54** has been actuated. In the event that it has, then as represented at line **552** and block **554**, the program enters the RIGS mode and, as represented at line **556** and block **558**, the RIGS mode display **56** is illuminated. The program then returns, as represented by line **560**, to line **340** at FIG. 6A. Where the inquiry at block **550** results in a negative determination, then as represented at loop line **762**, the program returns to line **476**.

An aspect of scanning in the RIGS procedure with probes as at **12** not only presides in a longstanding desire on the part of surgeons to carry out the procedure accurately, but as swiftly as possible. Thus, it is desirable to scan at an optimum rate across tissue but without failing to identify neoplastic tissue. Accordingly, the traditional probe control programs will collect valid photon event counts for very short intervals and evaluate those intervals in some form of a procedure. If the intervals themselves are too lengthy, then lower count rates emanating from subtle or very faint neoplastic sites may be filtered out and lost. This is a situation sometimes encountered in systems employing a moving average filter. To address these operational aspects, the present scanning system utilizes a short, 50 millisecond scan interval and collects successive ones of the counts for each such 50 millisecond scanning interval in temporary memory, and more particularly in circular buffer memory. The system then returns and looks at predetermined combinations of the memory contained 50 millisecond memory segments and compares these combinations of memory segment counts with a threshold which has been statistically computed with respect to each segment and combination of memory segments. With the arrangement, very small or occult sites of tumor are detected during the evaluation of the earlier or last in circular memory segment counts. To avoid an oversensitivity, a predetermined number of threshold crossings are required for each sweep or scan of these combinations of memory segment counts. This system and procedure is illustrated in connection with the flow chart set forth as in connection with FIGS. 8A and 8B. These figures should be considered in an orientation described by the labeling thereon.

Looking to FIG. 8A, the RIGS scanning program commences as represented at block **630** with an initialization of all variables and with initialization of such hardware components as necessary. Block **630** is provided with the assumption that the practitioner will have carried out a background count for the RIGS procedure in conjunction with the actuation of button **48** as described in connection with FIG. 2. As such, the program will acquire a threshold factor,  $f$  of **3**. This value is somewhat related to an election of three standard deviations (3 sigma). Next, as represented at line **632** and block **634** the temporary memory or circular buffer is cleared. Referring momentarily to FIG. 9, a circular buffer memory is stylistically depicted at **636**. The buffer memory **636** is configured having 15 bins or segments, each holding count values collected during a 50 millisecond scan interval. Thus, a memory segment count representing sequentially collected 50 millisecond intervals of counts extends from the most recently collected 50 ms count to the fifteenth next previous such count. In this regard, the memory segment counts at bin **638a** represent the counts at the latest acquired 50 ms scan interval and that segment retains an acquired count sum. By contrast, the fifteenth previous 50 millisecond interval count collection is at bin **638o**. With the circular memory approach, the memory segment count at bin **638o** will be discarded upon the

generation of the next memory segment count at bin **638a**. In conventional fashion, the memory count segments essentially rotate the extent of one segment with each acquisition of a memory segment count. The instant program accesses this circular memory **636** in a predetermined set of memory segment count combinations. A total of six such combinations are preferred for this scanning or sweeping form of analysis. In this regard, the program will sequentially look at the memory segment count at the most recent segment **638a**. Then, the program will look at a combination of memory segment counts at combined bins **638a** and **638b**. As labeled in FIG. 9, this represents a 100 millisecond duration, T, count collection. Next, the program will look at the combination of the memory segment counts at bins **638a**, **638b** and **638c**. For each of these combinations, the total count sum is divided by the time duration, T, represented by the number of segments. For example, the total count sum represented at bins **638a** and **638b** is divided by 100 milliseconds to obtain count rate, a value referred to by the acronym "ACRRV" meaning "ACQUIRED COUNT RATE RIGS VALUE." In a preferred software architecture, six sequential combinations are scanned, i.e., a combination commencing at bin **638a** and extending through bin **638f**. This amounts to an evaluation of up to 300 milliseconds of data collection.

Returning to FIG. 8A, following the clearing of the circular buffer, the program continues as represented at line **640** and block **642** wherein two timing functions or timers and counter of the program are initialized. The program then continues as represented at line **644** and block **646** wherein a timer, t1, is started or restarted. Then, as represented at line **648** and block **650** a second timer, t2, which is utilized for the noted scan interval is started or restarted. The program then continues as represented at line **652** and decision block **654**. The query posed by block **654** is one in which a determination is made as to whether a computed threshold has been crossed for a predetermined number, for example, three of the six combinations of memory segment counts as they are converted to count rates, for example in counts per second (CPS). The RIGS threshold is computed for each scan interval, for example, of 50, 100, 150, 200, 250 and 300 milliseconds. This computation is made in accordance with the following expression:

$$THRESHOLD = \frac{CEIL[(RBCV * T) + (f \sqrt{(RBCV * T)})]}{T} \quad (1)$$

Where:

RBCD = The RIGS background count value  
in CPS Units.

T = The count period used to calculate each  
ACRRV in units of seconds

CEIL = Ceiling function output results in the least  
integer value which is greater, or equal to,  
the input, i.e., the next higher integer value is  
selected if an integer value is not computed.

f is a threshold factor which is analogous to  
the number of statistical standard deviations.

Where: RBCD=The RIGS background count value in  
CPS Units.

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units of seconds

CEIL=Ceiling function output results in the least integer  
value which is greater, or equal to, the input, i.e., the  
next higher integer value is selected if an integer value  
is not computed.

f is a threshold factor which is analogous to the number  
of statistical standard deviations.

The query posed at decision block **654** requires the following:

$$\text{Any three ACRRVs} > \text{Threshold} \quad (2)$$

Recall that the initialization threshold factor, f, is set at **3**. In the event of an affirmative determination with respect to the query posed at block **654**, then as represented at line **656** and block **658**, an audible output is generated. The program then continues, as represented at line **660** and block **662**, to set the RIGS threshold factor, f, from a value of three to a value of one. The latter value is analogous to one statistical standard deviation or sigma. The program then continues as represented by line **662**, node **666** and line **668**.

Returning to block **654**, where the conditions of expression (2) are not met, then as represented at line **670** and block **672**, the audible sound is turned off. In this regard, it is important both to turn the sound on when the probe **12** window **16** is over a locator and to turn it off when the window **16** passes beyond the locator concentration. Upon turning the alarm off, then as represented at line **674** and block **676**, the threshold factor, f, is set back to the higher value of three. The program then continues as represented at line **678**, node **666** and line **668**.

Line **668** reappears in FIG. 8B. Looking to that figure, the line **668** extends to a node **680**. From that node **680**, a line **682** extends to the query posed at decision block **684**. This query determines whether the timer, t2, has reached or exceeded the scan interval, Tscan. It may be recalled that this interval preferably is of 50 ms duration. In the event of a negative determination with respect to this query, then the program dwells as represented by loop line **686** until the termination of the scan interval of 50 ms. Then, as represented at line **688** and block **690**, the circular buffer is updated. In this regard, as noted in FIG. 9, the most recent scan interval count value is inserted in bin **638a** and the value from fifteenth bin **638o** is discarded and replaced with the value in bin **638n**. The program then continues as represented at line **692** to the query posed at decision block **694**. This query determines whether or not the timer, t1, is equal to or greater than an updating interval, Tupdate. This interval preferably is one-half second and is the updating interval for displaying "cumulative" count rate values at location **80** of window **42** as described in connection with FIG. 2. In the event of a negative determination, then as represented at line **696**, the program loops to the restart block **650** shown in FIG. 8A. In the event of an affirmative determination indicating that display updating is appropriate, then, as represented at line **698** and block **700**, the program retrieves 0.75 seconds worth of memory segment counts from the circular memory. This is the entire 15 segment capacity of the memory. It may be recalled, however, that the update interval is one half second. Upon collecting the count sum from the 15 memory segments, then as represented at line **702** and block **704**, the count rate in counts per second is derived by straightforward division. The program then continues, as represented at line **706** and block **708**, to display the computed count rate. Finally, the program returns as represented by loop line **710** which extends to block **646** in FIG. 8A to restart timer, t1.

Since certain changes may be made in the above described system, apparatus, and method without departing

from the scope of the invention herein involved, it is intended that all matter contained in the description thereof or shown in the accompanying drawings, shall be interpreted as illustrative and not in a limiting sense.

What is claimed is:

1. A system for detecting and locating sources of radiation at a region of interest evidencing background radiation, comprising:

a probe moveable within said region of interest to provide a scan pulsed output corresponding with said sources and positionable to evaluate said background radiation and derive a background pulsed output corresponding therewith;

an audible indicator responsive to an audio input for providing an audibly perceptible output;

a signal treatment network responsive to validate said scan pulsed output and said background pulsed output to provide respective scan count signal and background count signals;

a background switch actuatable to provide a background activation signal;

a control circuit including temporary memory, responsive to said background activation signal and to said background count signals to derive a background count value, BCV, responsive to compile said scan count signals for a sequence of scan intervals to derive a scan interval count value with respect to each scan interval and locate said scan interval count values in said sequence in said temporary memory as memory segment counts, responsive for each said scan interval to access an initial select number of said memory segment counts in predetermined sequential memory segment count combinations, each said combination having a combined count period, T, responsive to said background value, BCV, to a first threshold factor, f1, and said combined count period, T, to compute a first count rate threshold value for each said count combination in correspondence with the expression:

$$\frac{(BCV * T) + (f1\sqrt{BCV * T})}{T},$$

responsive to generate said audio input when a predetermined number of said sequential memory segment count combinations represent a count rate greater than the corresponding said first count rate threshold value, responsive for a next said scan interval when said audio output has been generated to access a next select number of said memory segment counts in predetermined sequential memory segment count combinations, each said combination having a combined count period, T, responsive to said background value, BCV, to a second threshold factor, f2, less than said first threshold factor, f1, and said combined count period to compute a second count rate threshold value for each said count combination in correspondence with the expression:

$$\frac{(BCV * T) + (f2\sqrt{BCV * T})}{T},$$

responsive to generate said audio input when a predetermined number of said sequential memory segment count combinations represent a count rate greater than the corresponding said second count rate threshold value.

2. The system of claim 1 in which said control circuit is responsive to terminate said generated audio input when less

than said predetermined number of said sequential memory segment count combinations represent a count rate greater than the corresponding said second count rate threshold value.

3. The system of claim 1 in which said temporary memory is a circular buffer memory having at least a six memory segment capacity; and

said predetermined memory segment count combinations comprise:

(a) a first memory segment count corresponding with the most current one of said sequence of scan intervals, (b) said first memory segment count in combination with the next previous thereto second memory segment count, (c) said first memory segment count in combination with said second memory segment count and the next previous thereto third memory segment count, (d) said first memory segment count in combination with said second memory segment count, said third memory segment count and the next previous thereto fourth memory segment count, (e) said first memory segment count in combination with said second memory segment count, said third memory segment count, said fourth memory segment count and the next previous thereto fifth memory segment count, and (f) said first memory segment count in combination with said second memory segment count, said third memory segment count, said fourth memory segment count, said fifth memory segment count and the next previous thereto sixth memory segment count.

4. The system of claim 1 in which each said scan interval has a duration of about 50 milliseconds.

5. The system of claim 1 in which said initial select number of said memory segment counts is six.

6. The system of claim 1 in which said next select number of said memory segment counts is six.

7. The system of claim 1 in which:

said temporary memory is a circular buffer memory having a predetermined count display number of memory segments each retaining a said scan interval count value;

including a visually perceptible readout responsive to a rate signal to display a count rate readout; and

said control circuit is responsive at the timeout of successive update intervals to access said predetermined count display number of memory segments and derive said rate signal in correspondence with the combination of each said scan interval count value then retained by said circular buffer memory.

8. The system of claim 7 in which:

said circular buffer memory is a first in-last out buffer memory wherein each said memory segment represents a scan interval of 50 milliseconds: and

said predetermined number of memory segments is 15.

9. The system of claim 8 wherein said update interval is 500 milliseconds.

10. The system of claim 1 in which said first threshold factor, f1, is three.

11. The system of claim 1 in which said second threshold factor, f2, is one.

12. The system of claim 1 in which said expression deriving said first count rate threshold value is modified by a ceiling function altering said value to a next higher integer value when said first count rate threshold value is a non-integer value.

13. The system of claim 1 in which said expression deriving said second count rate value is modified by a ceiling

function altering said value to a next higher integer value when said second count rate threshold is a non-integer value.

**14.** A method for detecting and locating sources of radiation at a region of interest evidencing background radiation, comprising:

- (a) providing a probe movable within said region of interest;
- (b) positioning said probe at said region of interest for a background interval to derive a background pulsed output;
- (c) scanning said probe within said region of interest to derive a scanned pulsed output;
- (d) providing an audible indicator responsive to an audio input for providing an audibly perceptive output;
- (e) providing a signal treatment network responsive to validate said scan pulsed output and said background pulsed output to provide respective scan count signals and background count signals;
- (f) providing a control circuit including a circular memory having a predetermined number of memory bins from first to last;
- (g) deriving a background count value (BCV), from said background pulsed output;
- (h) compiling said scan output signals for a sequence of scan intervals to derive a scan interval count value with respect to each scan interval;
- (i) locating each said scan interval count value as a memory segment count in said sequence in sequential said memory bins;
- (j) for each compiled said scan interval, accessing a first predetermined number of combinations of said memory bins which include said first bin and the corresponding count period, T, represented by each of said combinations, and computing a first count rate threshold value for each said combination in correspondence with the expression:

$$\frac{(BCV * T) + (f1\sqrt{BCV * T})}{T},$$

where f1 is a first threshold factor;

- (k) deriving said audio input when a predetermined first number of said combinations represent a count rate greater than the said first count rate threshold value corresponding therewith;
- (l) for the compiled next scan interval following said compiled scan interval of step (j), when said audio input has been derived in step (k), accessing a second predetermined number of combinations of said memory bins and the corresponding count period, T, represented by each of said combinations, and computing a second count rate threshold value for each said combination in correspondence with the expression:

$$\frac{(BCV * T) + (f2\sqrt{BCV * T})}{T},$$

where f2 is a second threshold factor less than said first threshold factor; and

- (m) deriving said audio input when a predetermined second number of said combination derived in step (l) represent a count rate greater than the said second count rate threshold value corresponding therewith.

**15.** The method of claim 14 including the step:

- (n) terminating said derived audio input when less than said predetermined second number of said combinations derived in step (h) represent a count rate greater than said second count rate threshold value corresponding therewith.

**16.** The method of claim 14 in which:

said step (j) includes the step of modifying the said first count rate threshold value to a next higher integer value when said first count rate threshold value is a non-integer value.

**17.** The method of claim 14 in which:

said step (l) includes the step of modifying the said second count rate threshold value to a next higher integer value when said second count rate threshold value is a non-integer value.

**18.** The method of claim 14 in which said first threshold factor, f1, is three.

**19.** The method of claim 14 in which said second threshold factor, f2, is one.

**20.** A system for detecting and locating sources of radiation at a region of interest within an environment evidencing background radiation, comprising:

- a probe movable within said region of interest to provide a scan pulsed output corresponding with radiation from said sources and positionable to evaluate said background radiation and derive a background pulsed output corresponding therewith;
- an audible indicator responsive to an audio input for providing an audibly perceptive output;
- a signal treatment network responsive to validate said scan pulsed output and said background pulsed output to provide respective scan count signal and background count signals;
- a background switch actuable to provide a background activation signal;
- a control circuit including temporary memory, responsive to said background activation signal and to said background count signals to derive a background value, responsive to compile said scan count signals for a sequence of scan intervals to derive a scan interval count value with respect to each of said scan intervals and locate said scan interval count value in said sequence in said temporary memory as memory segment counts, responsive for each said scan interval to access a select number of said memory segment counts in predetermined memory segment count combinations to derive a corresponding select number of scanned count rate values, responsive to said background value, to a first statistically significant threshold factor and each scan interval represented by said memory segment count combinations to derive a first count rate threshold value for each of said combinations responsive to generate said audio input when a predetermined number of corresponding said combinations represent a count rate greater than a corresponding said first count rate threshold value, then responsive for a next said scan interval when said audio output has been generated, to access a select number of said memory segment counts in predetermined memory segment count combinations to derive a corresponding select number of scanned count rate values, responsive to said background value, to a second statistically significant threshold factor less than said first threshold factor and each scan interval represented by said memory count combinations to derive a second count rate threshold

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value for each said combination, responsive to generate said audio output when a predetermined number of corresponding said combinations represent a count rate greater than said second count rate threshold value.

21. The system of claim 20 in which said temporary memory is a circular buffer memory having at least a six memory segment capacity; and

said predetermined memory segment Count combinations comprise: (a) a first memory segment count corresponding with the most current one of said sequence of scan intervals, (b) said first memory segment count in combination with the next previous thereto second memory segment count, (c) said first memory segment count in combination with said second memory segment count and the next previous thereto third memory segment count, (d) said first memory segment count in combination with said second memory segment count, said third memory segment count and the next previous thereto fourth memory segment count, (e) said first memory segment count in combination with said second memory segment count, said third memory segment count, said fourth memory segment count and the next previous thereto fifth memory segment count, and (f) said first memory segment count in combination with said second memory segment count, said third memory segment count, said fourth memory segment count, said fifth memory segment count and the next previous thereto sixth memory segment count.

22. The system of claim 20 in which said control circuit select number of memory segment counts is six and said predetermined number of scanned count rate values is three.

23. The system of claim 20 in which said control circuit is responsive for said next scan interval to access said select number of said memory segment counts wherein said select number is six.

24. The system of claim 23 in which said control circuit is responsive to terminate said audio input when fewer than three of said scanned count rate values are greater than said second threshold count rate value.

25. The system of claim 24 in which said control circuit is responsive to generate said audio output when three of said corresponding select number of scanned count rate values represent count rates greater than said second threshold count rate value.

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26. The system of claim 20 in which:

said temporary memory is a circular buffer memory having a predetermined count display number of memory segments each for retaining a said scan interval count value;

including a visually perceptible readout responsive to a rate signal to display a count rate readout; and

said control circuit is responsive at the timeout of successive update intervals to access said predetermined count display number of memory segments and derive said rate signal in correspondence with the combination of each said scan interval count value then retained by said circular buffer memory.

27. The system of claim 26 in which:

said circular buffer memory is a first in-last out buffer memory wherein each said memory segment represents a scan interval of 50 milliseconds; and

said predetermined count display number of memory segments is 15.

28. The system of claim 27 wherein said update interval is 500 milliseconds.

29. The system of claim 20 in which:

said first statistically significant threshold factor is three; and

said second statistically significant threshold factor is one.

30. The system of claim 20 in which said signal treatment network comprises:

an energy window network including a lower threshold operational amplifier having a lower threshold reference value and responsive to said scan and background pulse outputs to validate the minimum energy values thereof; and

a pulse width discriminator for validating only those scan and background pulse outputs having pulse widths below a pulse width value representing noise.

31. The system of claim 30 in which said pulse width discriminator is responsive to validate said pulse widths of said pulse outputs in correspondence with said lower threshold reference value.

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