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(54) **MICROFLUIDIC DEVICES, SYSTEMS, AND METHODS FOR QUANTIFYING PARTICLES USING CENTRIFUGAL FORCE**

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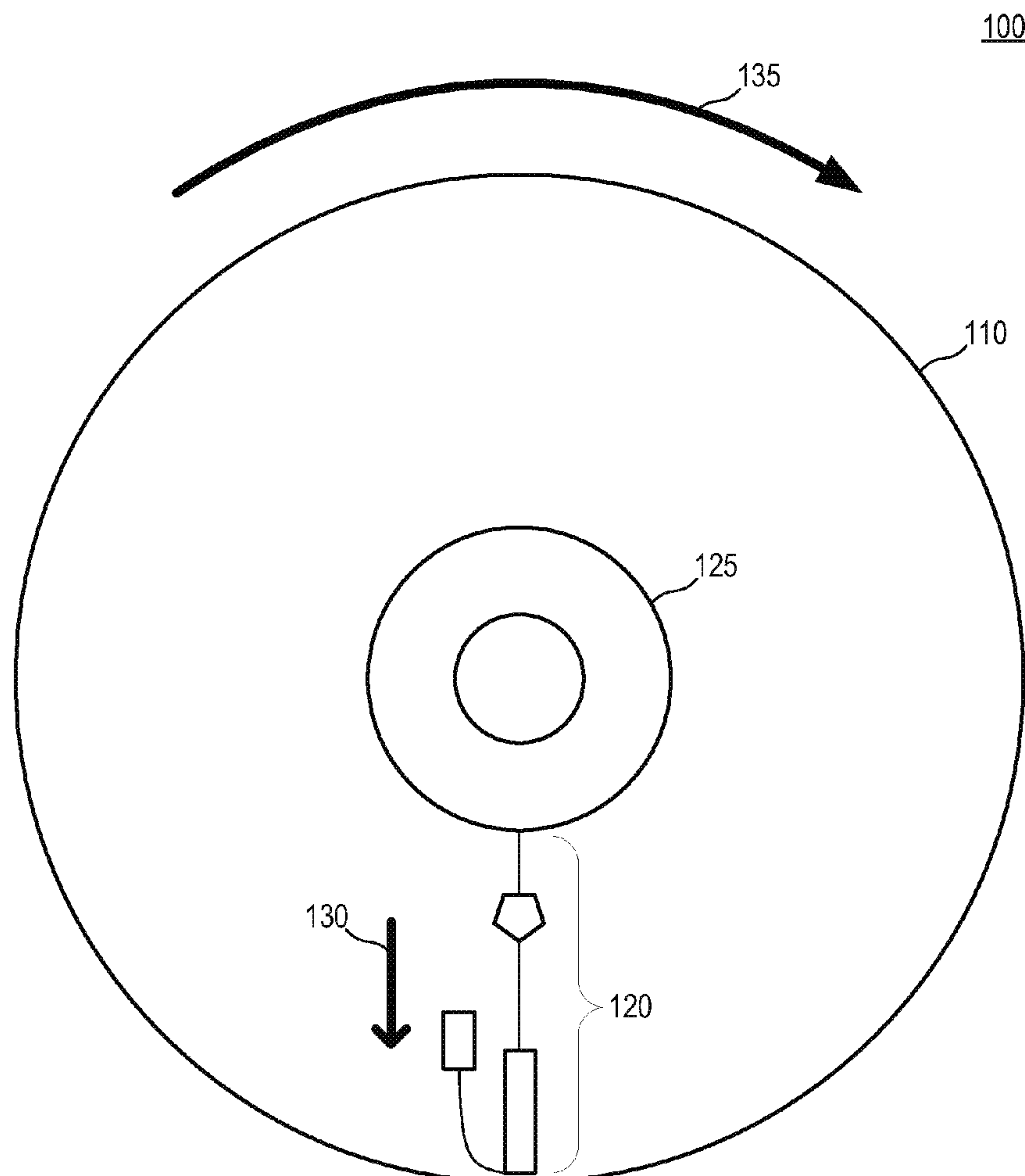
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(57) **ABSTRACT**

Embodiments of the present invention are directed toward microfluidic systems, apparatus, and methods for measuring a quantity of cells in a fluid. Examples include a differential white blood cell measurement using a centrifugal microfluidic system. A method may include introducing a fluid sample containing a quantity of cells into a microfluidic channel defined in part by a substrate. The quantity of cells may be transported toward a detection region defined in part by the substrate, wherein the detection region contains a density media, and wherein the density media has a density lower than a density of the cells and higher than a density of the fluid sample. The substrate may be spun such that at least a portion of the quantity of cells are transported through the density media. Signals may be detected from label moieties affixed to the cells.



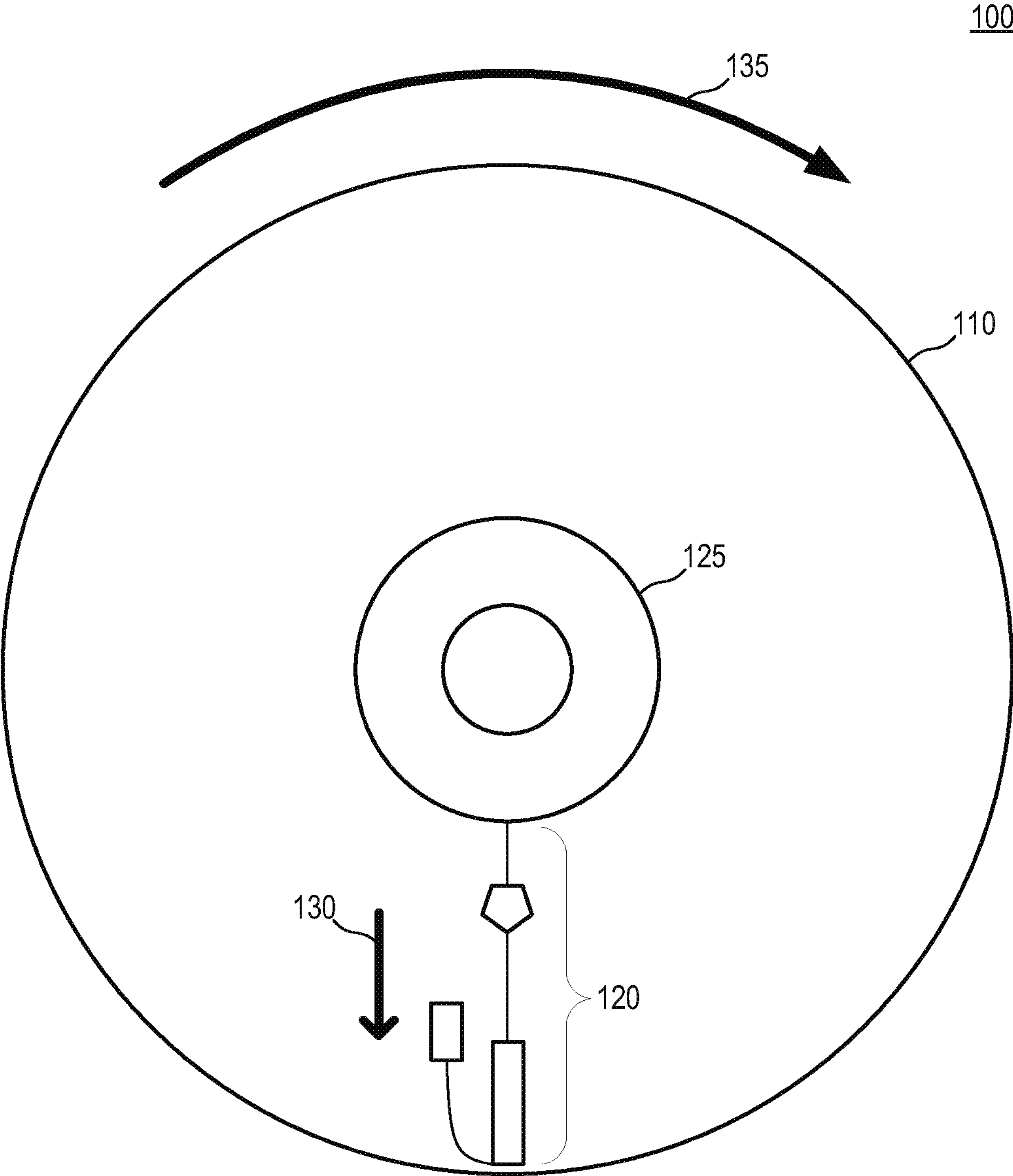


Figure 1

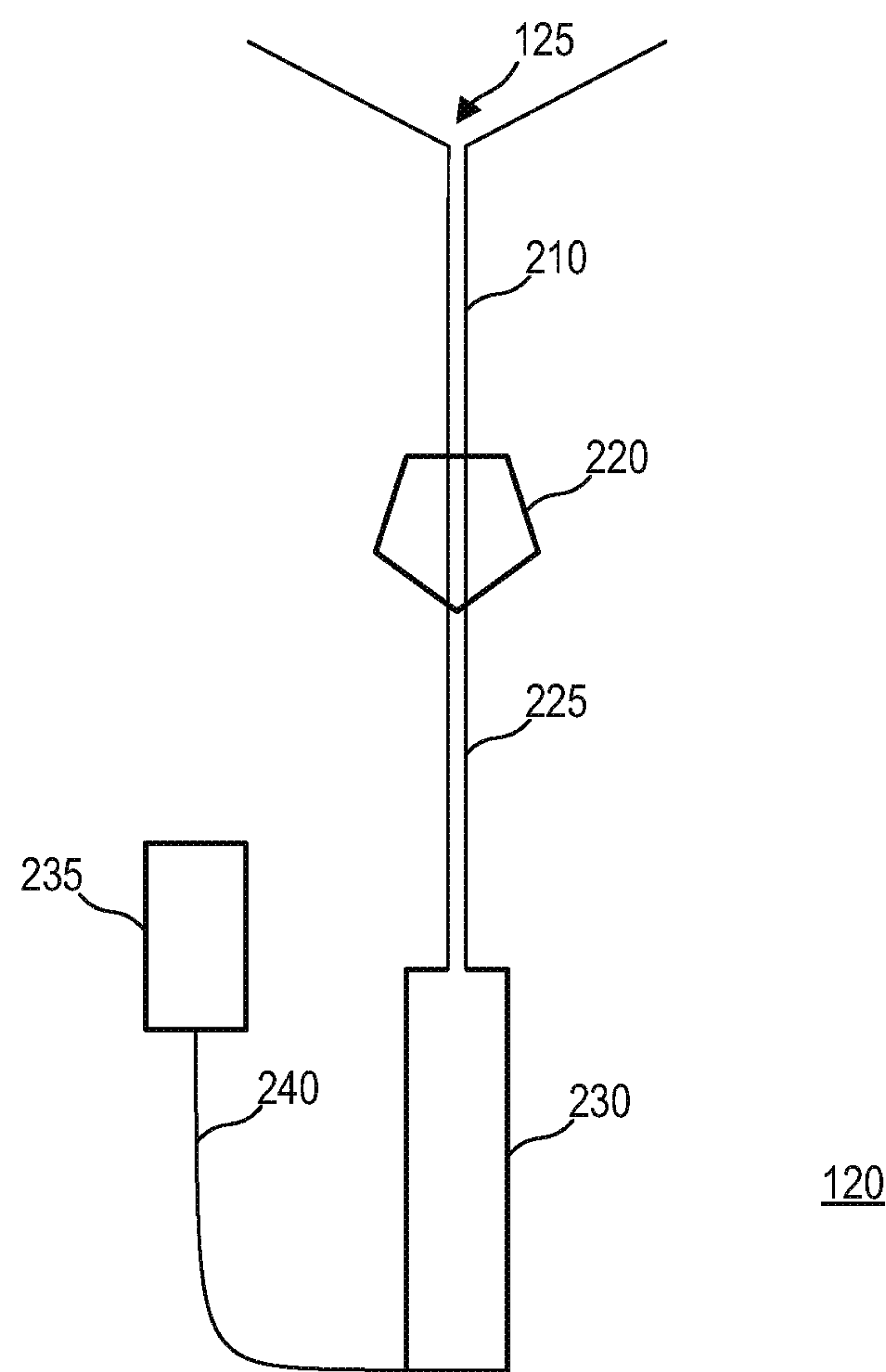


Figure 2

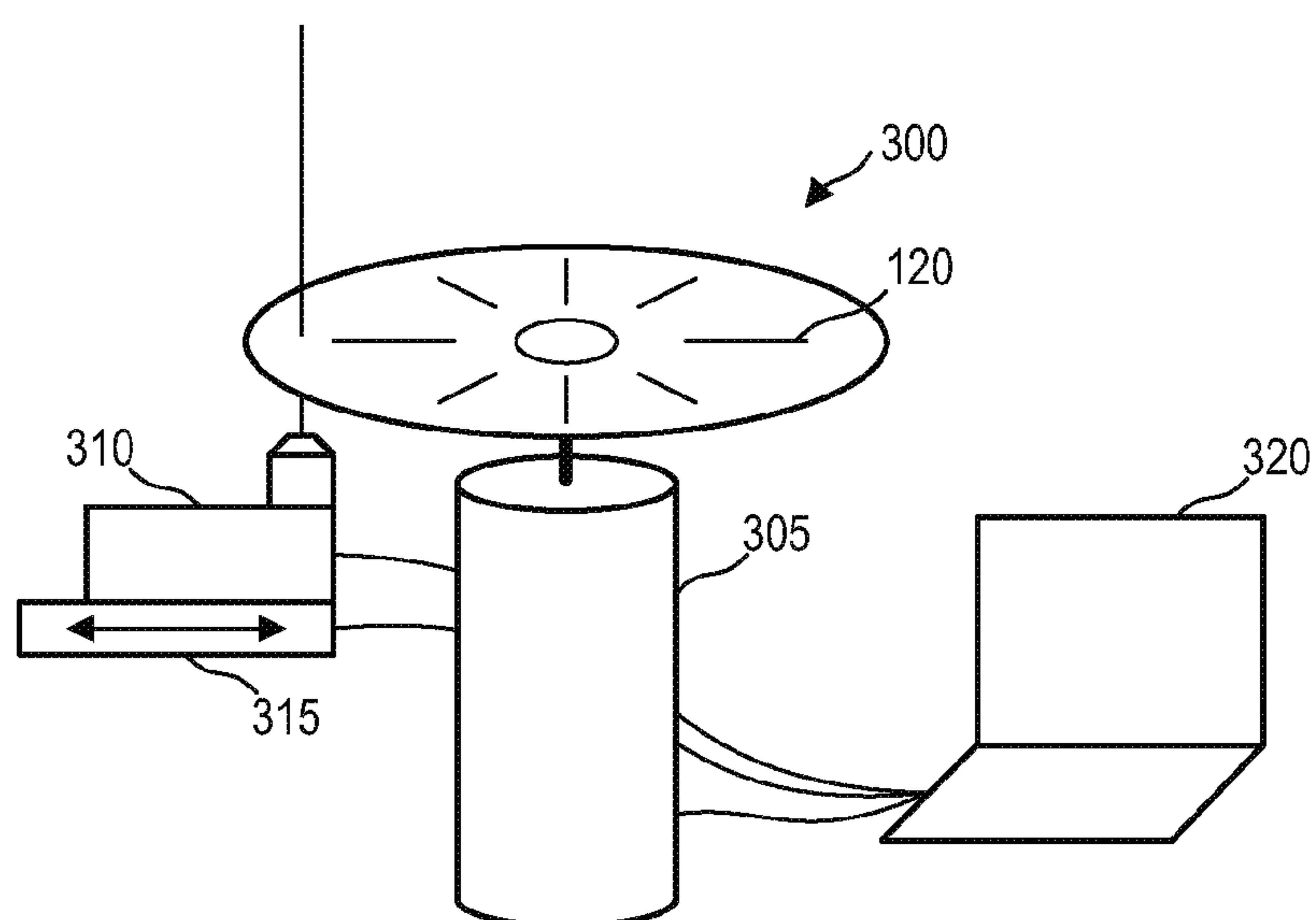


Figure 3

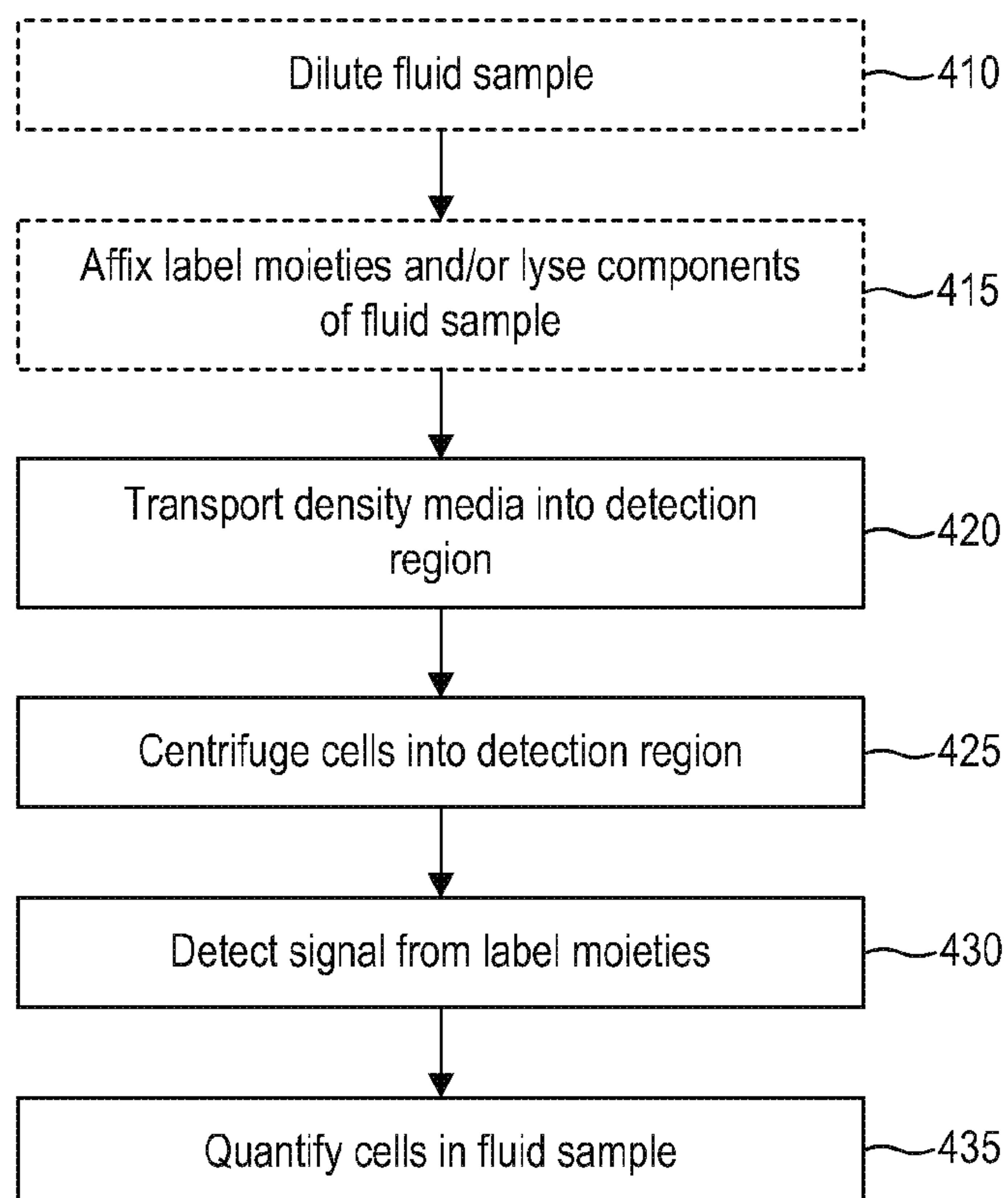


Figure 4

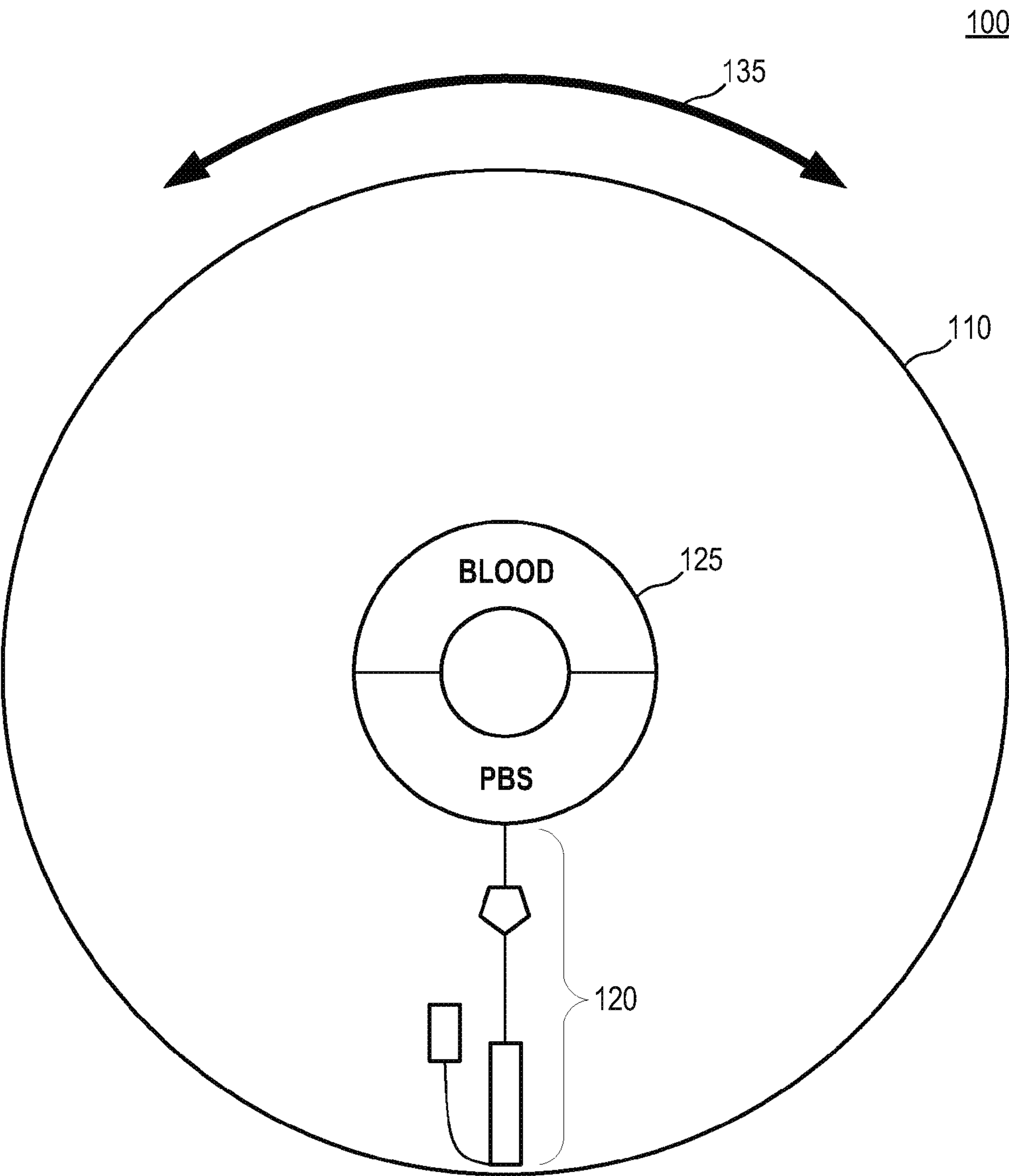


Figure 5

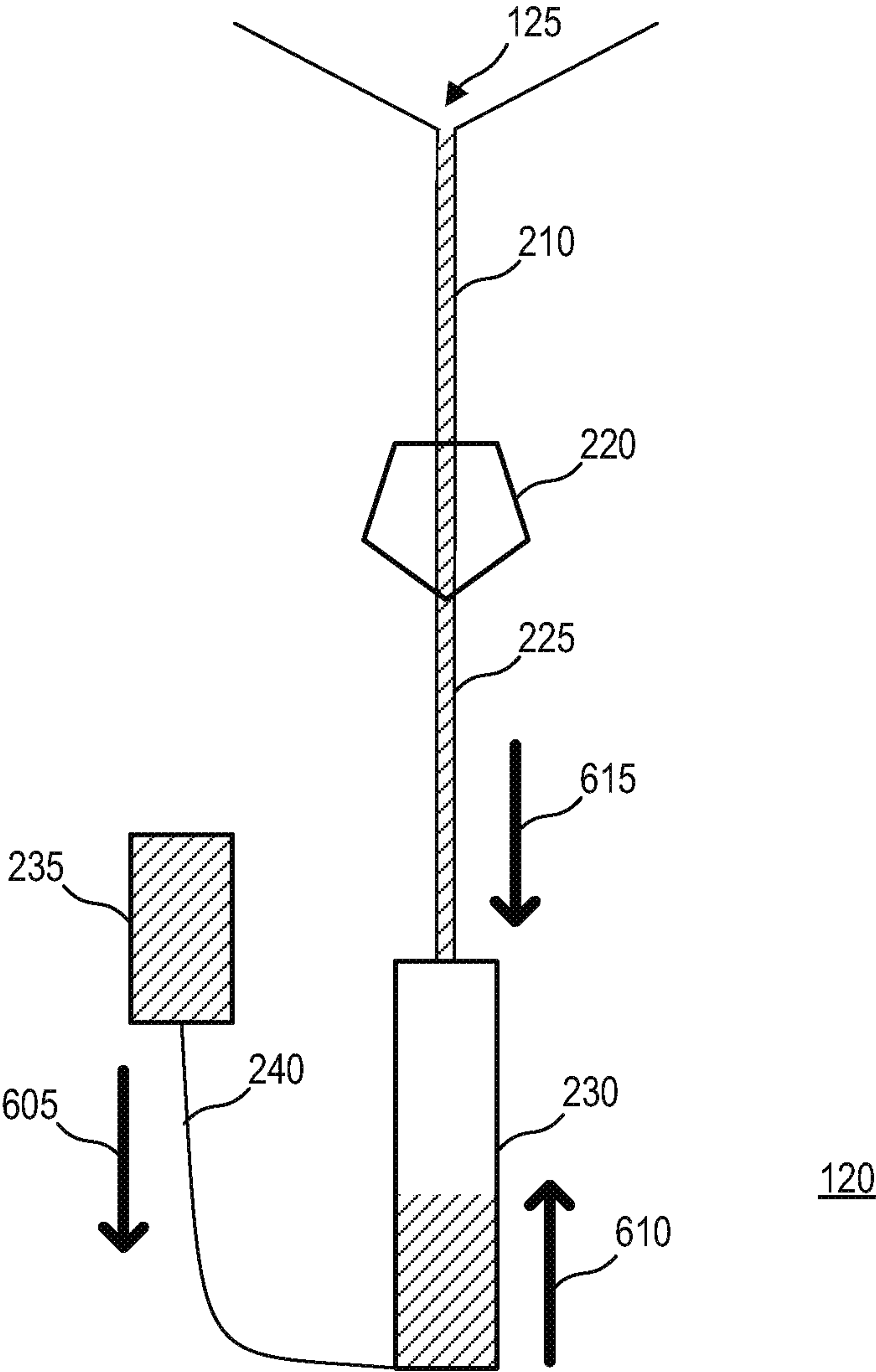


Figure 6

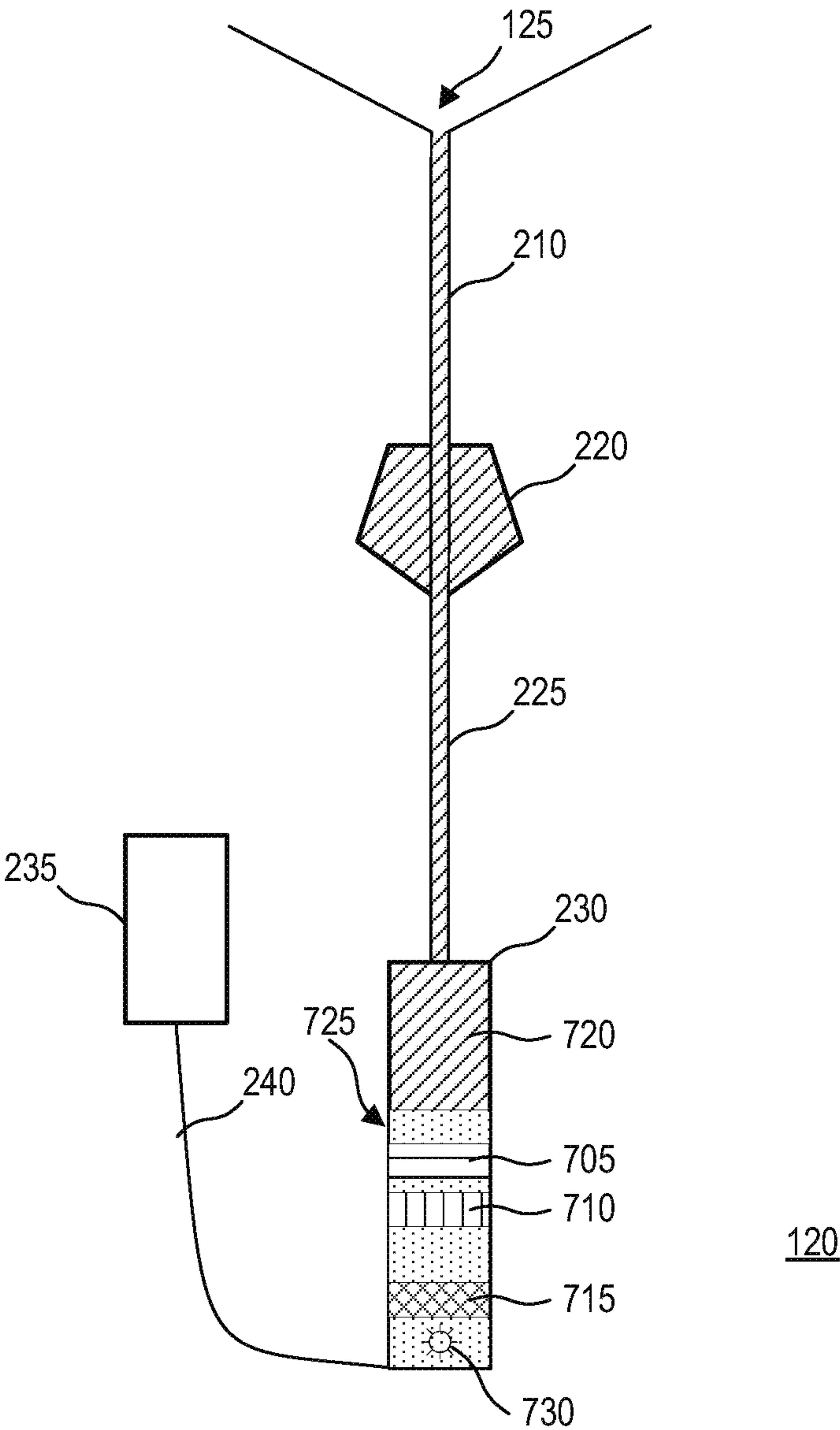


Figure 7

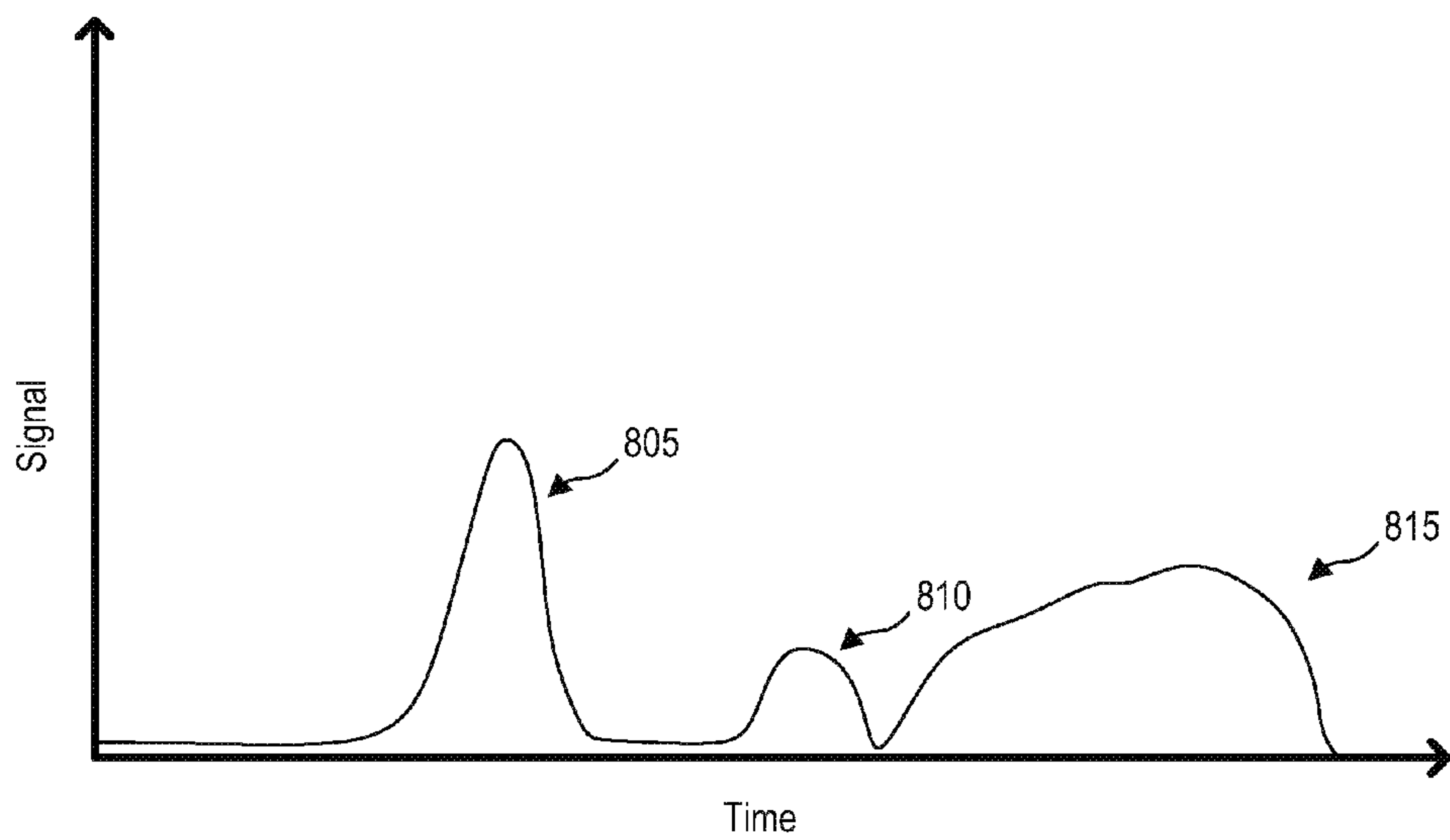


Figure 8

Figure 9

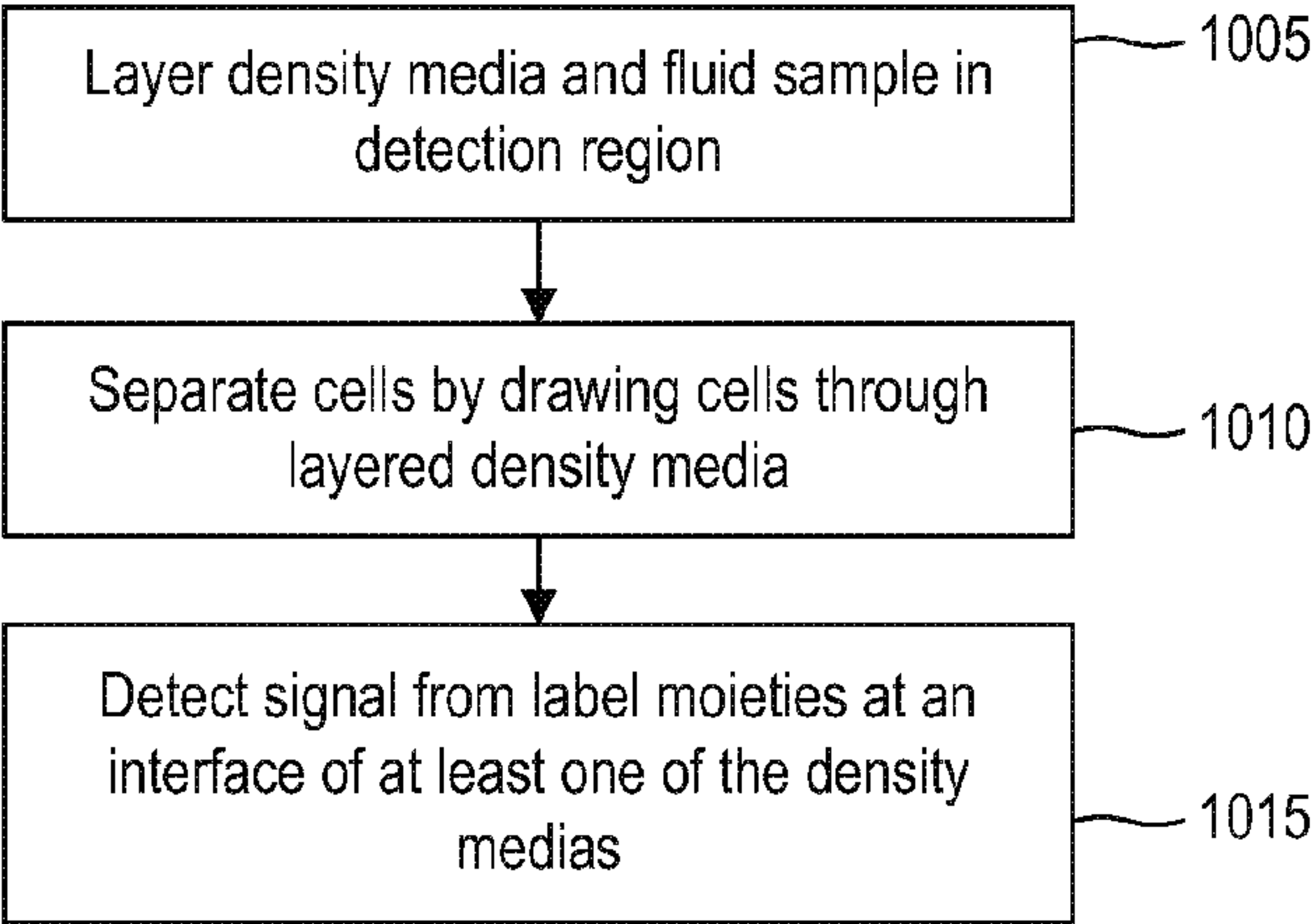
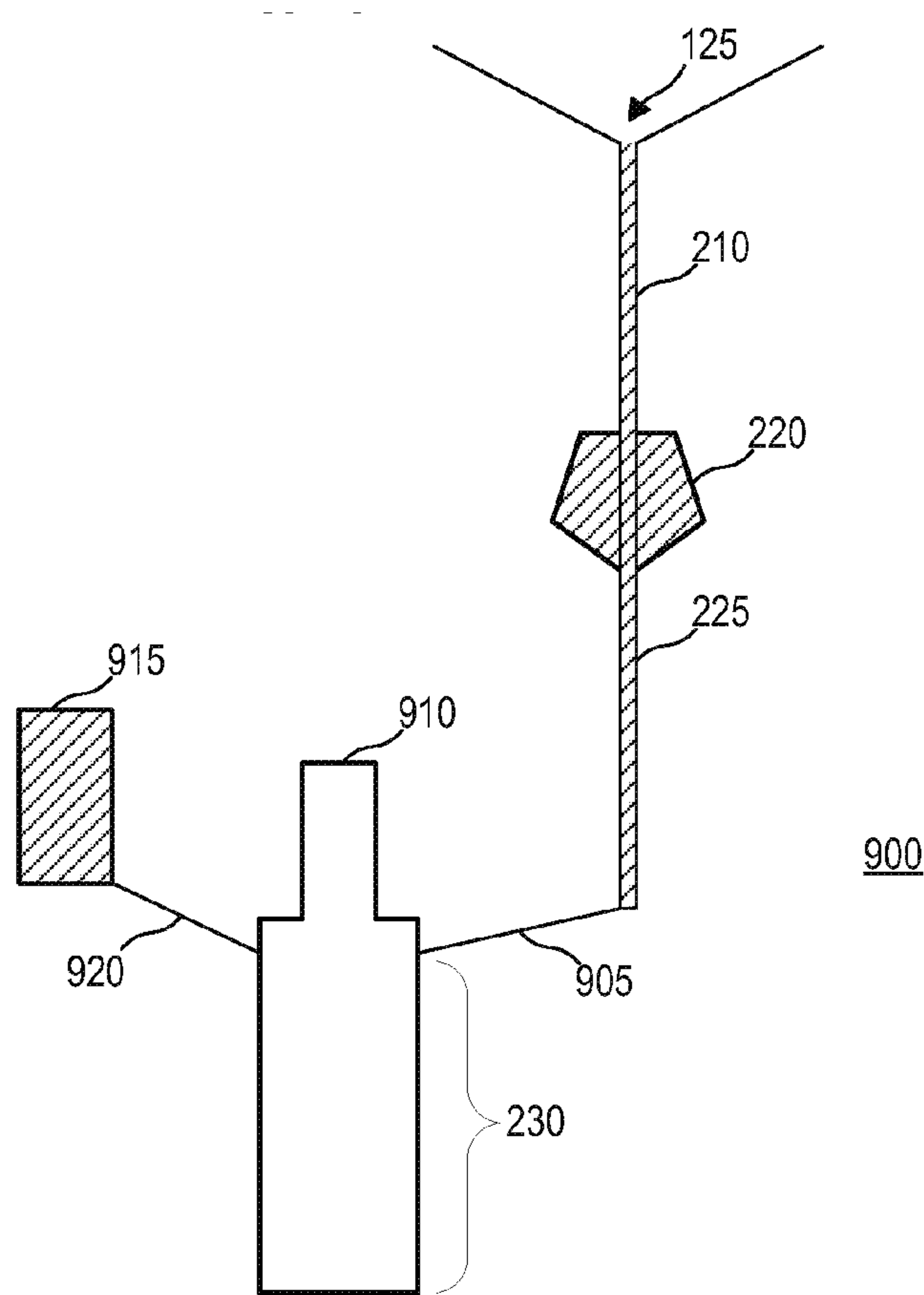


Figure 10

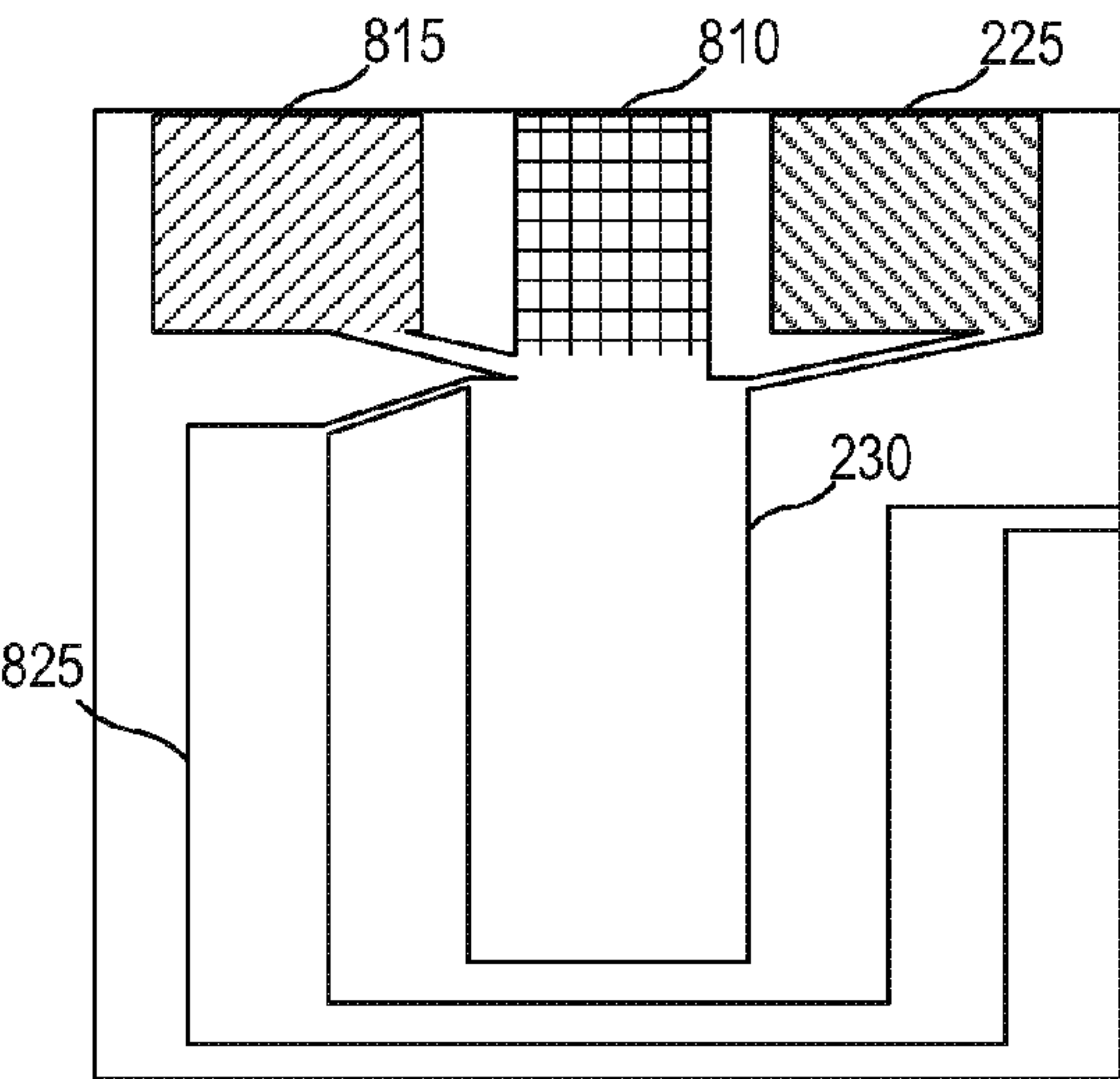


Figure 11

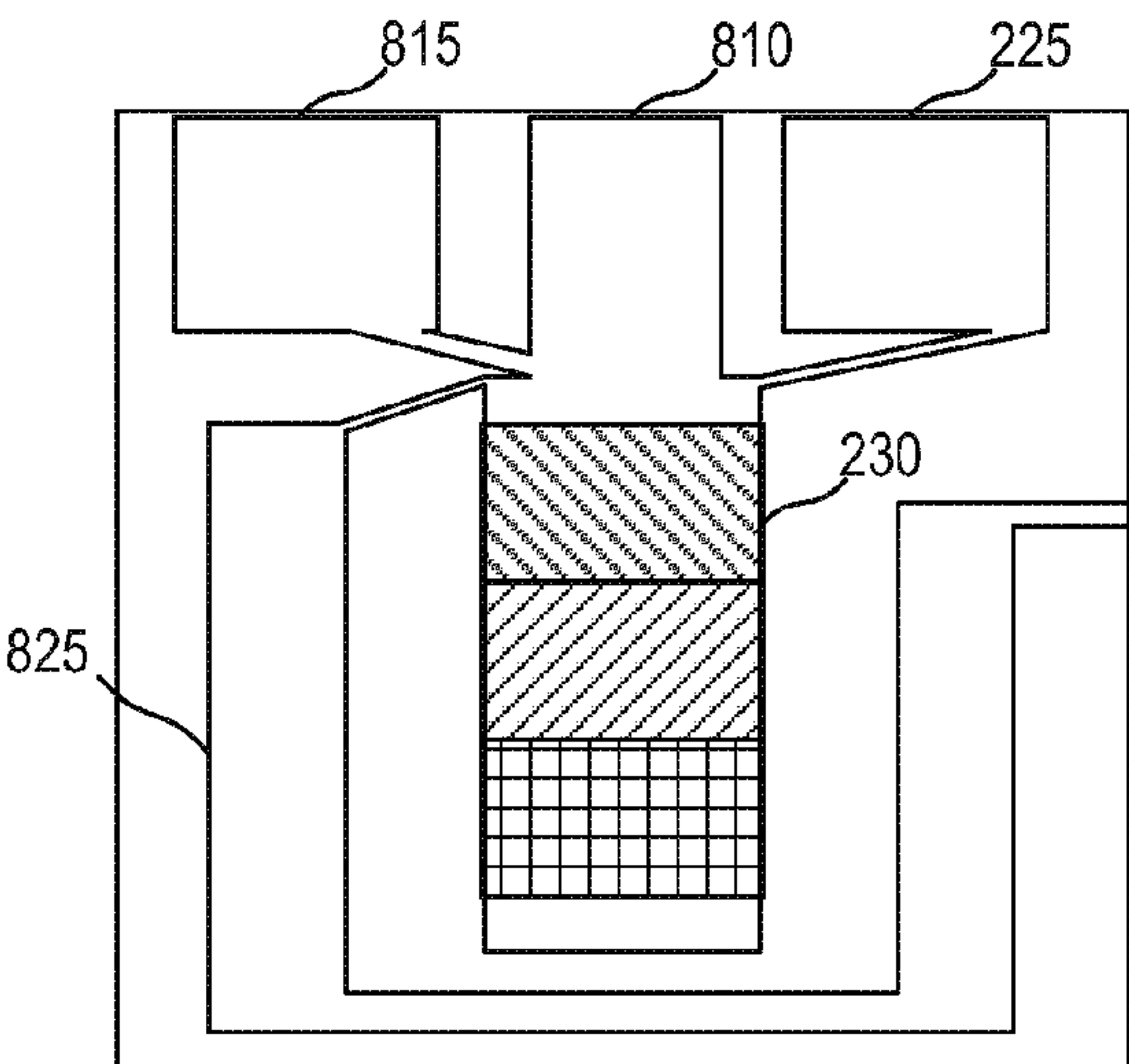


Figure 12

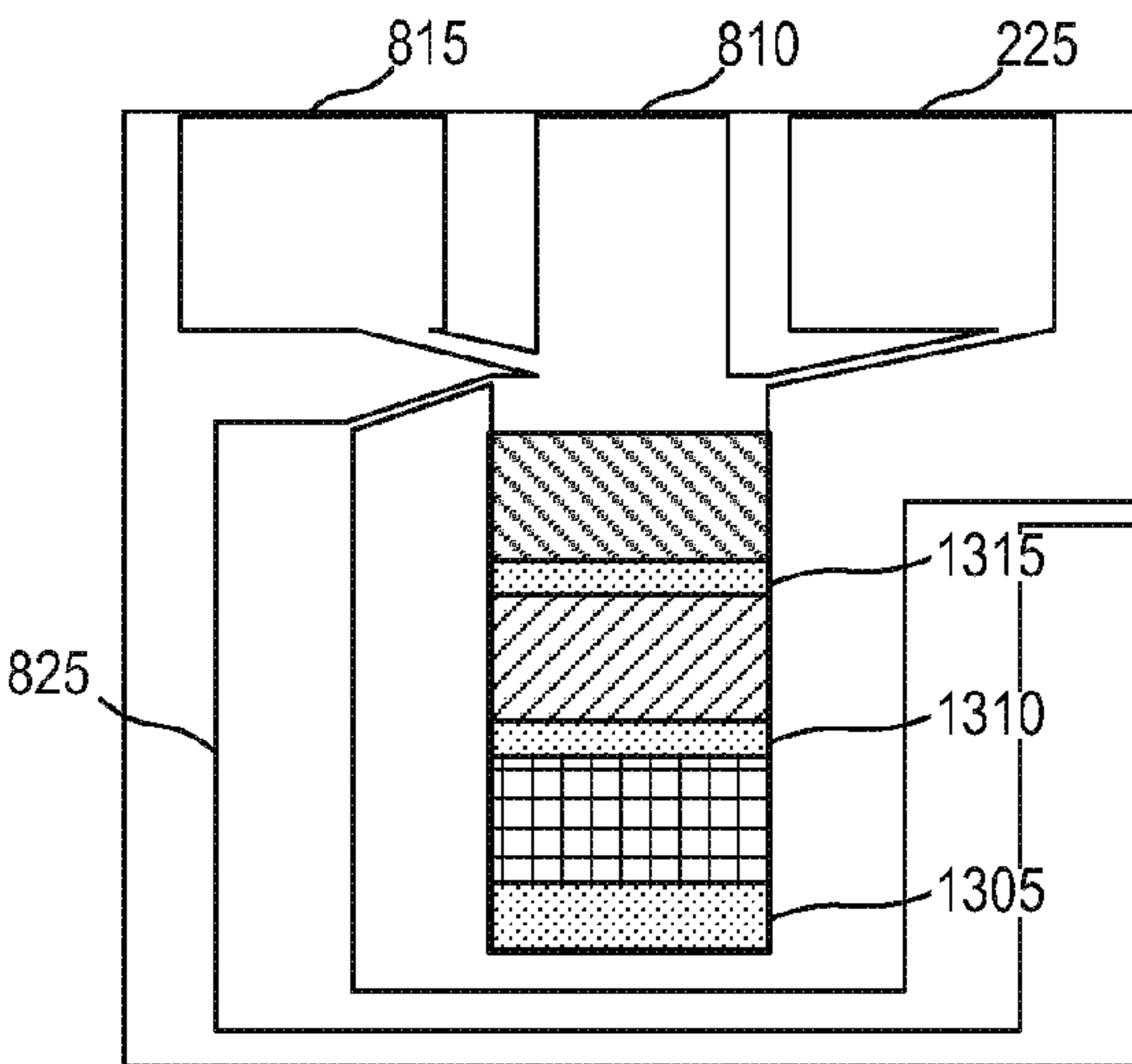


Figure 13

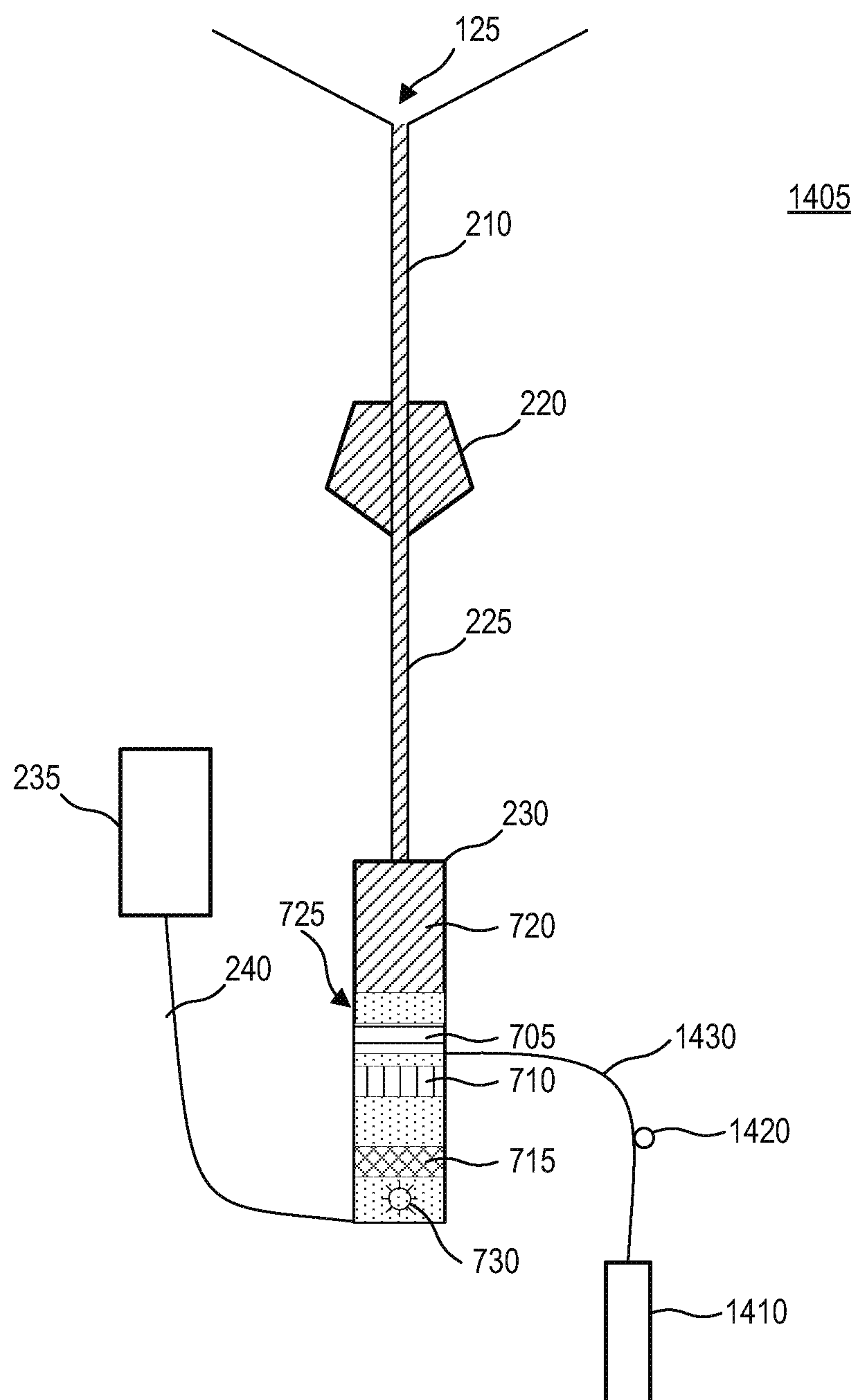


Figure 14

MICROFLUIDIC DEVICES, SYSTEMS, AND METHODS FOR QUANTIFYING PARTICLES USING CENTRIFUGAL FORCE

CROSS-REFERENCE TO RELATED APPLICATION(S)

[0001] This application is a divisional application of, and discloses subject matter that is related to subject matters disclosed in, co-pending parent application U.S. Ser. No. 12/891,956, filed Sep. 28, 2010 and entitled “MICROFLUIDIC DEVICES, SYSTEMS, AND METHODS FOR QUANTIFYING PARTICLES USING CENTRIFUGAL FORCE” which claims the benefit of the earlier filing date of U.S. Provisional Application 61/351,458, filed Jun. 4, 2010, entitled “Method for Counting White Blood Cells”. The present application claims the priority of the aforementioned applications which are hereby incorporated by reference, in their entirety, for any purpose.

STATEMENT REGARDING RESEARCH & DEVELOPMENT

[0002] Described examples were made with Government support under Government Contract No. DE-AC04-94AL85000 awarded by the U.S. Department of Energy to Sandia Corporation. The Government has certain rights in the invention, including a paid-up license and the right, in limited circumstances, to require the owner of any patent issuing in this invention to license others on reasonable terms.

TECHNICAL FIELD

[0003] Embodiments of the invention relate generally to centrifugal microfluidic systems and examples include methods, systems, and apparatus employing centrifugal forces for quantifying particles in fluid.

BACKGROUND

[0004] A variety of diagnostic techniques utilize a cell count from a fluid sample, such as a differential white blood cell count. For example, a differential white blood cell count may be utilized in medical diagnostic techniques for detecting sepsis, leukemia, AIDS, radiation exposure, as well as other conditions. Typical methods for measuring white blood cell count include flow cytometry, electrical impedance counting, and visual counting from a fluid sample under a microscope. See, for example, Holmes, D., et. al. “Leukocyte analysis and differentiation using high speed microfluidic single cell impedance cytometry,” *Lab Chip* 9, 2881-2889 (2009), which article is hereby incorporated by reference in its entirety for any purpose. These commonly used techniques may require a large fluid sample for analysis, and may occur as a stand-alone diagnostic procedure. Further, the techniques may require operation by a skilled technician.

[0005] Microfluidic systems, including “lab on a chip” or “lab on a disk” systems continue to be in development. See, Lee, B. S., et. al., “A fully automated immunoassay from whole blood on a disc,” *Lab Chip* 9, 1548-1555 (2009) and Madou, M. et. al., “Lab on a CD,” *Annu. Rev. Biomed. Engr.* 8, 601-628 (2006), which articles are hereby incorporated by reference in their entirety for any purpose.

BRIEF DESCRIPTION OF THE DRAWINGS

[0006] FIG. 1 is a schematic illustration of a microfluidic disk arranged in accordance with embodiments of the present invention.

[0007] FIG. 2 is a schematic illustration of a cell quantification area of a microfluidic disk in accordance with an embodiment of the present invention.

[0008] FIG. 3 is a schematic illustration of a system according to an embodiment of the present invention.

[0009] FIG. 4 is a flowchart illustrating a method according to an embodiment of the present invention.

[0010] FIG. 5 is a schematic illustration of a microfluidic disk including blood and PBS in the fluid inlet port.

[0011] FIG. 6 is a schematic illustration of a cell quantification area showing directions of fluid flow in accordance with an embodiment of the present invention.

[0012] FIG. 7 is a schematic illustration of a cell quantification area showing separated cells in accordance with an embodiment of the present invention.

[0013] FIG. 8 is a schematic illustration of signal detected over time from labeled cells in accordance with an embodiment of the present invention.

[0014] FIG. 9 is a schematic illustration of another embodiment of a cell quantification area arranged in accordance with the present invention.

[0015] FIG. 10 is a flowchart illustrating an example method for measuring cells according to an embodiment of the present invention.

[0016] FIG. 11 is a schematic illustration of a portion of a cell quantification region in accordance with an embodiment of the present invention.

[0017] FIG. 12 is a schematic illustration of a portion of a cell quantification area following layering of density media.

[0018] FIG. 13 is a schematic illustration of a portion of a cell quantification region following cell separation of a whole blood sample.

[0019] FIG. 14 is a schematic illustration of a portion of a cell quantification area including a post-processing area in accordance with an embodiment of the present invention.

DETAILED DESCRIPTION

[0020] Certain details are set forth below to provide a sufficient understanding of embodiments of the invention. However, it will be clear to one skilled in the art that embodiments of the invention may be practiced without various of these particular details. In some instances, well-known chemical structures, chemical components, molecules, materials, electronic components, circuits, control signals, timing protocols, and software operations have not been shown in detail in order to avoid unnecessarily obscuring the described embodiments of the invention.

[0021] Embodiments of the present invention are directed toward microfluidic systems, apparatus, and methods for quantifying, e.g. counting, a quantity of particles in a fluid. Although examples are described with reference to the measurement of white blood cells and differential white blood cell counting, it is to be understood that other types of cells may also be quantified in an analogous manner. Indeed, in other examples, substantially any particles, including beads, having a characteristic volume and shape may be measured using examples described herein.

[0022] FIG. 1 is a schematic illustration of a microfluidic disk 100 arranged in accordance with embodiments of the

present invention. The microfluidic disk **100** may include a substrate **110** which may at least partially define regions of a cell quantification area **120**. The microfluidic disk **100** may include a fluid inlet port **125** in fluid communication with the cell quantification area **120**. During operation, as will be described further below, fluid, including a quantity of cells in the fluid, may be transported using centrifugal force from an interior of the microfluidic disk **100** toward a periphery of the microfluidic disk **100** in a direction indicated by an arrow **130**. The centrifugal force may be generated by rotating the microfluidic disk **100** in the direction indicated by the arrow **135**, or in the opposite direction.

[0023] The substrate **110** may be implemented using any of a variety of suitable substrate materials. In some embodiments, the substrate may be a quartz substrate. Quartz, glass, polycarbonate, fused-silica, PDMS, and other transparent substrates may be desired in some embodiments to allow optical observation of sample within the channels and chambers of the disk **100**. In some embodiments, however, a plastic, metal or semiconductor substrate may be used. In some embodiments, multiple materials may be used to implement the substrate **110**. The substrate **110** may include surface treatments or other coatings, which may in some embodiments enhance compatibility with fluids placed on the substrate **110**. In some embodiments surface treatments or other coatings may be provided to control fluid interaction with the substrate **110**. While shown as a round disk in FIG. 1, the substrate **110** may take substantially any shape, including square.

[0024] The substrate **110** may generally, at least partially, define a variety of microfluidic features. Generally, microfluidic, as used herein, refers to a system, device, or feature having a dimension of around 1 mm or less and suitable for at least partially containing a fluid. In some embodiments, 500 μm or less. In some embodiments, the microfluidic features may have a dimension of around 100 μm or less. Other dimensions may be used. The substrate **110** may define one or more microfluidic features, including any number of channels, chambers, inlet/outlet ports, or other features.

[0025] Microscale fabrication techniques, generally known in the art, may be utilized to fabricate the microfluidic disk **100**. The microscale fabrication techniques employed to fabricate the disk **100** may include, for example, embossing, etching, injection molding, surface treatments, photolithography, bonding and other techniques.

[0026] A fluid inlet port **125** may be provided to receive a fluid that may be analyzed using the microfluidic disk **100**. The fluid inlet port **125** may have generally any configuration, and fluid may enter the fluid inlet port **125** utilizing substantially any fluid transport mechanism, including dropping, pipetting, or pumping a fluid sample into the fluid inlet port **125**. The fluid inlet port **125** may take substantially any shape. Generally, the fluid inlet port **125** is in fluid communication with the cell quantification area **120**. Generally, by fluid communication it is meant that a fluid may flow from one area to the other, either freely or using one or more transport forces and/or valves, and with or without flowing through intervening structures.

[0027] The cell quantification area **120** will be described further below, and generally may include one or more microfluidic channels in fluid communication with the fluid inlet port **125**. Although a single cell quantification area **120** is shown in FIG. 1, generally any number may be present on the microfluidic disk **100**.

[0028] As the microfluidic disk **100** is rotated in the direction indicated by the arrow **135** (or in the opposite direction), a centrifugal force may be generated. The centrifugal force may generally transport fluid from the inlet port **125** through the cell quantification area **120**.

[0029] FIG. 2 is a schematic illustration of a cell quantification area **120** of a microfluidic disk in accordance with an embodiment of the present invention. The cell quantification area **120** includes a microfluidic channel **210** in fluid communication with the fluid inlet port **125**. A reservoir **220** is in fluid communication with the microfluidic channel **210**. The reservoir **220** is in fluid communication with a detection region **230** via a channel **225**. Another reservoir **235** is in fluid communication with the detection region **230** via a channel **240**.

[0030] The reservoirs **220** and **235** may generally be implemented using any size and shape, and may contain one or more reagents including solids and/or fluids which may interact with fluid entering and/or exiting the reservoir. In some examples, the reservoir **220** is configured to hold lysis agents and/or label moieties. The label moieties may be selected to affix to the cells for quantification. That is, the label moieties may bind or otherwise become affixed to cells and may emit a signal suitable for detection, such as an optical or an electrical signal. For example, to quantify white blood cells, a membrane permeable DNA-specific fluorescent dye may be used, such as lyophilized DNA dye. Many suitable dyes are available, including but not limited to LDS-751. See Maes, M. L., et. al., "Comparison of sample fixation and the use of LDS-751 or anti-CD45 for leukocyte identification in mouse whole blood for flow cytometry," *J. Immunol. Methods* 319, 79-86 (2007), which article is hereby incorporated by reference in its entirety for any purpose. In other examples, labeled antibodies that recognize proteins on the surface of specific cells may be used. Cells labeled in this manner may be separated by size and density as described herein and may be detected using signal detected from the labeled antibodies. For example, a label moiety may include an antibody against CD14 chemically coupled to a fluorescent label moiety. The CD14 label moiety may then bind to monocytes. Utilizing label moieties specific to one or more particular cell types may aid in the quantification of the labeled cell type relative to others having similar size and/or density, such as but not limited to, T-lymphocytes and/or B-lymphocytes. In some examples, lipid dye molecules may be used as label moieties. Blood cell membranes include lipid bilayers, and lipid dye molecules may accordingly be used as label moieties in some examples. Lipid dye molecules may facilitate detection and/or quantification of red blood cells and platelets in addition to white blood cells in some examples. The lysis agents may include, for example, a detergent such as Saponin for the lysis of red blood cells.

[0031] The reservoir **235** may be configured to contain a liquid density media. The density media may have a density lower than a density of the cells to be quantified and higher than a density of the fluid sample. The density media may generally be implemented using a fluid having a density selected to be in the appropriate range—lower than a density of the cells to be quantified and higher than a density of the fluid sample. In some examples, a fluid sample may be diluted for use with a particular density media. The density media may include, for example, a salt solution containing a suspension of silica particles which may be coated with a bio-compatible coating. An example of a suitable density media is

Percoll™, available from GE Lifesciences. Particular densities may be achieved by adjusting a percentage of Percoll™ in the salt solution. Generally, viscosity and density of the density media may be adjusted by selecting a composition of the media. Varying the concentration of solutes such as sucrose or dextran in the media may adjust the density and/or viscosity.

[0032] A table of example densities of particular blood components is provided below in Table 1.

TABLE 1

Example densities of blood components	
Component	Density
Whole Blood	1.06
Plasma	1.025
Red blood cells	1.095
Granulocytes	1.085
Monocytes	1.07
Lymphocytes	1.07

[0033] Accordingly, a suitable density media to quantify white blood cells in accordance with examples of the present invention (including granulocytes, monocytes, and lymphocytes) may have a density between 1.06 and 1.07. In some examples, a whole blood sample may be diluted to a lower density to allow for a larger range of acceptable density media. In one example, a whole blood fluid sample may be diluted using a salt solution, such as PBS, to a density of around 1.03. A suitable density media may then have a density between about 1.03 and 1.07. For example, a density media having a density of 1.06 may be used.

[0034] The detection region **230** may be a channel or chamber and may vary in configuration in accordance with the detection technique employed, as will be described further below. The detection region **230** may generally be configured to allow for detection of a signal emitted by label moieties affixed to the cells to be quantified.

[0035] As will be described further below, centrifugal forces may generally be used to transport a fluid sample including cells to be quantified from the inlet port **125** toward the detection region **230**. Additionally, centrifugal forces may be used to transport density media from the reservoir **235** to the detection region **230**.

[0036] FIG. 3 is a schematic illustration of a system according to an embodiment of the present invention. The system **300** may include the disk **100** of FIG. 1 with one or more cell quantification areas **120**. A motor **305** may be coupled to the disk **100** and configured to spin the disk **100**, generating centrifugal forces. A detection module **310** may be positioned to detect signal from label moieties in a detection region of the cell quantification area **120**, as will be described further below. An actuator **315** may be coupled to the detection module **310** and configured to move the detection module along the detection region in some examples. A processing device **320** may be coupled to the motor **305**, the detection module **310**, and/or the actuator **315** and may provide control signals to those components. The processing device **320** may further receive electronic signals from the detection module **310** corresponding to the label moiety signals received by the detection module **310**. All or selected components shown in FIG. 3 may be housed in a common housing in some examples. Microfluidic disks may be placed on the motor **305** and removed, such that multiple disks may be analyzed by the system **300**.

[0037] The motor **305** may be implemented using a centrifugation and/or stepper motor. The motor **305** may be positioned relative to the detection module **310** such that, when the disk **100** is situated on the motor **305**, the disk is positioned such that a detection region of the cell quantification area **120** is exposed to the detection module **310**.

[0038] The detection module **310** may include a detector suitable for detecting signal from label moieties affixed to cells to be quantified. The detector may include, for example, a laser and optics suitable for optical detection of fluorescence from fluorescent labels. In other examples, other detectors, such as electronic detectors, may be used. The actuator **315** may move the detector in some examples where signal may be detected from a variety of locations of the microfluidic disk **100**, as will be described further below.

[0039] In other examples, although not explicitly shown in FIG. 3, one or more actuators may be coupled to the motor **305** and/or disk such that the disk is moved relative to the detection module responsive to signals from the processing device, as will be described further below.

[0040] The processing device **320** may include one or more processing units, such as one or more processors. In some examples, the processing device **320** may include a controller, logic circuitry, and/or software for performing functionalities described herein. The processing device **320** may be coupled to one or more memories, input devices, and/or output devices including, but not limited to, disk drives, keyboards, mice, and displays. The processing device may provide control signals to the motor **305** to rotate the disk **100** at selected speeds for selected times, as will be described further below. The processing device may provide control signals to the detection module **310**, including one or more detectors and/or actuators, to detect signals from the label moieties and/or move the detector to particular locations, as will be described further below. The processing device may develop these control signals in accordance with input from an operator and/or in accordance with software. The software may include instructions encoded one or more memories configured to cause the processing device to output a predetermined sequence of control signals. The processing device **320** may receive electronic signals from the detection module **310** indicative of the detected signal from label moieties. The processing device **320** may quantify cells in a fluid sample based on the signals received from the detection module **310**, as will be described further below. Accordingly, the processing device **320** may perform calculations as will be described further below. The calculations may be performed in accordance with software including one or more executable instructions stored on a memory causing the processing device to perform the calculations. Results may be stored in memory, communicated over a network, and/or displayed. It is to be understood that the configuration of the processing device **320** and related components is quite flexible, and any of a variety of computing systems may be used including server systems, desktops, laptops, controllers, and the like.

[0041] Having described examples of microfluidic disks and systems in accordance with embodiments of the present invention, methods for quantifying a number of particles in a fluid sample will now be described. Some discussion will also be provided regarding mechanisms for sedimentation and centrifugation. The discussion regarding mechanisms is provided as an aid to understanding examples of the present invention, but is in no way intended to limit embodiments of

the present invention. That is, embodiments of the present invention may not employ the described mechanisms.

[0042] Sedimentation of spheres may occur within a viscous fluid under the influence of a gravitational field (which may be natural or induced by centrifugation). The settling velocity of approximately spherical particles, such as cells, may be described by Stoke's flow equations:

$$V_s = \frac{2}{9} \frac{(\rho_p - \rho_f)}{\mu} g R^2;$$

[0043] where V_s is the sedimentation velocity, μ is the fluid viscosity, ρ_p is the density of the particle, ρ_f is the density of the fluid, g is acceleration due to effective gravity, and R is the particle radius. Note that sedimentation rate scales with the square of particle radius and therefore a small difference in cell radius may form a basis for separation of cells in some examples, as the cells may sediment at a different rate. There is also a linear dependence of sedimentation rate with the difference in density between the particle and the surrounding fluid, which may also be an effective mechanism for separation. Accordingly, cells or other particles may be separated according to their density and/or radius, as the cells will have different sedimentation velocities. Separation of cells using these principles may be referred to as "rate zonal centrifugation."

[0044] Table 1, above, provided example densities of components of whole blood and various components. Table 2, below, includes example diameter, in microns, of those components.

TABLE 1

Example diameters of blood components	
Component	Diameter (microns)
Whole Blood	N/A
Plasma	N/A
Red blood cells	2.5-7
Granulocytes	8
Monocytes	8.5
Lymphocytes	6.5

[0045] FIG. 4 is a flowchart illustrating a method according to an embodiment of the present invention. In block **410** a fluid sample including a quantity of particles may be diluted. Block **410** may be followed by block **415** in which sample preparation of the fluid sample may occur. For example, in block **415** label moieties may be affixed to the quantity of particles. Alternatively or in addition, in block **415**, components of the fluid sample may be lysed. Block **415** may be followed by block **420**. In block **420**, density media may be transported into a detection region of a microfluidic disk. Block **420** may be followed by block **425**. In block **425**, the quantity of particles in the fluid sample may be transported toward the detection region using centrifugal force. The quantity of particles may be transported through the density media. Block **425** may be followed by block **430**. In block **430**, signal may be detected from the label moieties affixed to the quantity of cells. Block **430** may be followed by block **435**. In block **435**, the quantity of cells may be quantified using the signal detected from the label moieties.

[0046] In block **410** a fluid sample may be diluted. The fluid sample may be introduced to a microfluidic disk, such as the disk **100** of FIGS. 1 and 2 before or after dilution. Any of a variety of suitable fluid samples may be used including, but not limited to, whole blood, buffer solutions, saliva, urine, cerebrospinal fluid, mixed cell culture, tissue homogenates, or other biological fluid samples. Generally, the fluid sample will include a quantity of particles, such as cells, to be measured in accordance with embodiments of the present invention. As has been described above, in one example, whole blood may be diluted to a density less than that of a density media used. In one example, a density media having a density of 1.06 is used while the whole blood may be diluted to a density of 1.03 using a 1:1 dilution with a salt solution such as PBS. FIG. 5 is a schematic illustration of the microfluidic disk **100** including blood and PBS in the fluid inlet port **125**. The microfluidic disk may be spun, for example using the motor **305** of FIG. 3, such that the blood and PBS solution are mixed in block **410** of FIG. 4. In other examples, a fluid sample may be diluted or otherwise mixed prior to introduction to the microfluidic disk **100**.

[0047] In block **415**, any of a variety of sample preparation operations may occur. For example, label moieties may be affixed to cells in the fluid sample and/or components of the fluid sample may be lysed. Referring back to FIG. 2, in some examples, label moieties and/or lysing agent(s) may be contained in the chamber **220**. The microfluidic disk **100** may be spun, for example using the motor **305** of FIG. 3, such that the fluid sample including a quantity of cells are transported into and/or through the chamber **220**. The fluid sample including the quantity of cells may be transported continuously through the chamber **220** while lysis and/or labeling occur, or in some examples, the spinning of the microfluidic disk **100** may be stopped for a time to allow for labeling and/or lysis. Suitable lysis agents and label moieties have been described above. In some embodiments, particles may be bound to target analytes in the fluid sample, such as cells, for quantification of the target analyte. For example, particles made from silica, gold, iron oxide, or combinations thereof may be coated with an antibody for recognition of proteins on the surface of certain cells. Other particles may be used. The particles may be included in the mixing chamber **220** in some examples. The particles may bind to the certain cells and increase the sedimentation rate of certain cells on binding, allowing the certain cell types to be selectively removed from the sample during centrifugation for quantification and/or post-processing. Particles coated with molecules other than antibodies, such as integrins or selectins, may also be used for specific cell binding. In one example, silica beads coated with an antibody against the protein CD14 may be used to specifically bind to monocytes and cause the bound monocytes to sediment more quickly than other cell types.

[0048] In other examples, labeled antibodies that may recognize proteins on the surface of specific cells may be included in the chamber **220** in addition or instead of DNA labeling and/or lysis agents. Cells labeled in this manner may be separated by size and density, as described below, and the labeled cells may have additional labeling characters.

[0049] Referring back to FIG. 4, in block **420**, the density media may be transported into the detection region, such as the detection region **230** of FIG. 2. In some examples, density media may already be present in the detection region **230** and need not be transported in a separate operation. In some examples, the density media may be stored in the chamber

235. The microchannel **240** may have a width selected to serve as a valve, such that a spin rate over a threshold amount is required to initiate a flow of the density media **235** out of the chamber **235** through the microchannel **240**. In some examples, the microchannel **240** has a width and spin rates for one or more of blocks **410-415** are selected such that the density media is retained in the chamber **235** while the fluid sample is transported toward the detection region **230** through the chamber **220**. A spin rate of the microfluidic disk **100** may be increased at the block **420** to initiate or enhance a flow of the density media **235** into the detection region **230**. In this manner, the microchannel **240** may function as a valve. Other valve structures may be used in other examples. In block **420**, the valve may be activated to allow the flow of density media into the detection region **230**.

[0050] In block **425**, cells in the fluid sample may be centrifuged into the detection region. Centrifugal force may be used to continue to transport the fluid sample toward the detection region **230** of FIG. 2. The microfluidic disk **100** may be spun, using for example the motor **305** of FIG. 3, to transport the fluid sample containing a quantity of labeled cells into the detection region **230**.

[0051] FIG. 6 is a schematic illustration of the cell quantification area **120** showing directions of fluid flow in accordance with an embodiment of the present invention. The microfluidic disk **100** may be spun at a rate sufficient to cause the density media to be transported from the chamber **235** to the detection area **230** through the microfluidic channel **240** using centrifugal force. The density media accordingly may flow in the direction shown by arrows **605** and **610**. A fluid sample may be transported by the same centrifugal forces from the inlet **125** toward the detection region **230**, as shown by the arrow **615**.

[0052] As has been described above, the density media may have a density greater than that of the fluid sample, but lower than that of the cells to be quantified. Accordingly, as the flow of fluid sample indicated by the arrow **615** meets the flow of density media **610**, the cells from the fluid sample may be transported through the density media using centrifugal force, while remaining components of the fluid sample may not be transported through the density media. For example, hemoglobin spilled from red cell lysis may remain suspended and not transported through the density media due to in part to the smaller particle size compared to cells. Red blood cell membranes may remain suspended and not transported through the density media due to their lower density than the density media. Further, excess label moieties may not be transported through the density media. Labeled white blood cells, however, may be transported through the density media.

[0053] Referring back to FIG. 4, in block **430**, a signal may be detected from label moieties affixed to the cells. The signal may be detected in any of a variety of ways, and the detection methodology may be selected for compatibility with the label moiety and quantification technique described further below. In the case of a fluorescent label moiety, an optical detector may be used to detect fluorescence emitted by the label moieties. The rate at which labeled cells are transported through the density media may depend on the density and radius of the labeled cells, as was described above using theoretical principles. Accordingly, cells may be separated from the fluid sample based on their density and/or radius.

[0054] FIG. 7 is a schematic illustration of the cell quantification area **120** showing separated cells in accordance with an embodiment of the present invention. As the microfluidic

disk **100** spins and applies a centrifugal force to the fluid sample, cells may be separated by their radius and/or density into bands. Bands **705**, **710**, and **715** are shown in FIG. 7 within the detection region **230**. The band **705** may correspond to lymphocytes, the band **710** to monocytes, and the band **715** to granulocytes. Components of the fluid sample **720** which are less dense than the density media remain separated from the density media **725** in the detection region. In some embodiments, an optical detector, such as the detection module **310** of FIG. 3, may be positioned to detect signal from label moieties at a location **730**. As the separated labeled cell bands **705**, **710**, and **715** are transported through the density media toward the detection location **730**, they may be optically detected.

[0055] Table 3 below provides an average time to the detection location **730** for different cell types based on the 1.06 density media described above, whole blood diluted to a 1.03 density, and a detector positioned 4 mm from an interface between the whole blood fluid sample and the density media. A 12 cm diameter microfluidic disk is assumed, with a detection region 1 cm away from the edge of the disk.

TABLE 3

Example migration time of blood components in viscous media Media density = 1.06 Viscosity = 15 centipoise Spin rate = 5400 RPM	
Cell Type	Migration Time (s)
Red blood cells	66
Granulocytes	70
Monocytes	175
Lymphocytes	226

[0056] Note that, in some examples, red blood cells may not be present in the sample, and/or may have been lysed.

[0057] FIG. 8 is a schematic illustration of signal detected over time from labeled cells in accordance with an embodiment of the present invention. Referring back to FIG. 7, the granulocyte band **715** may be the first to pass the detection location **730**, generating a detected signal peak **805** in FIG. 8. The granulocyte band **715** is the first to reach the detection location at least because the granulocytes may be more dense than the monocytes and lymphocytes. The monocyte band **710** may be the next to reach the detection location, generating a detected signal peak **810**. The monocyte band **710** may reach the detection location after the granulocyte band **715** because the monocytes may be less dense than the granulocytes, as described above, and may have a larger diameter than the lymphocytes. The lymphocyte band **705** may then be the last to pass the detection location **730**, generating a detected signal peak **815**. In some examples, the peaks may overlap, for example, if the detection region is not long enough to allow for distinct separation of the peaks.

[0058] Referring again to FIG. 4, in block **435**, the detected cells may be quantified. The quantification may be based on the signal detected from the label moieties in block **430**, and any of a variety of quantification techniques may be used. The quantification may be performed, for example, by the processing device **320** of FIG. 3 based on signals received from the detection module **310**. Referring to FIG. 8, a total number of white blood cells may be quantified by integrating the signal received over time. A relative number of granulocytes,

monocytes, and/or lymphocytes may be calculated by integrating the respective signal peaks over time.

[0059] Following a sufficient amount of centrifugation, the labeled cells may accumulate in a pellet at the peripheral portion of the detection region **230** of FIG. **2**. That is, all labeled white blood cell components may eventually be driven to an outermost portion of the detection region **230** by centrifugal force. An absolute total cell count may be obtained by measuring the height of the pellet. The cells may occupy a volume consistent with random close packing of spheres, where the pellet may include 64 percent cells and 36 percent fluid-filled space. In examples where the cells may not approximate spheres, other percentages may be used. In this manner, a height of the pellet may be proportional to the total number of labeled cells. The pellet height may be measured, for example, by the detection module **310** of FIG. **3**, or by examination with a microscope or other signal detection apparatus. The total cell concentration may be calculated from the pellet height and detection region geometry as follows:

$$\text{CellConcentration} = \frac{0.64 * \text{Thickness} * \text{Width}}{\text{CellVolume} * \text{SampleSize}} * \text{PelletHeight},$$

[0060] where the Thickness and Width are dimensions of the detection region in which the pellet has formed. In one example, 2 μL of whole blood may be analyzed in a detection region which is 0.5 mm wide and 80 μm thick. An average white blood cell diameter may be 7.5 μm , and the sedimented pellet height of the white cell layer may be 86 μm . Accordingly, a white blood cell concentration of $5 \times 10^6/\text{mL}$ may be calculated.

[0061] In some examples, a red blood cell count may also be measured, along with a white blood cell count, in accordance with embodiments of the present invention. For example, referring back to FIG. **1**, an additional cell quantification area may be provided in addition to or instead of the cell quantification area **120**. The additional cell quantification area may not include a chamber for cell lysis, and accordingly, red blood cells may also be transported through the density media described above. The red cell pellet height following sedimentation may be used as described above to calculate a number or concentration of red blood cells. In this manner, both red and white blood cell counts may be obtained from a same microfluidic disk in some examples.

[0062] In some examples, a centrifugal force may be reduced or removed after one or more white blood cell components have been separated from the fluid sample as illustrated in FIG. **7**. Instead of transporting the bands **705**, **710**, **715** past a detection location **730**, a detector may be scanned along the detection region **230** to detect the bands **705**, **710**, **715**. For example, referring to FIG. **3**, the actuator **315** may move the detection module **310** along a length of the detection region on the microfluidic disk **100**. Signal may be detected from label moieties at different distances in the detection region, similar to the signal shown in FIG. **8**, except with the x axis representative of distance. In this manner, signal may be detected from the separated components, and an integral of the signal peaks may yield relative cell counts, as generally described above.

[0063] Accordingly, embodiments of devices, systems, and methods for measuring cells in a fluid sample have been described above. Embodiments described include transport-

ing a quantity of cells through a density media having a density that is greater than the fluid sample but less than a density of the cells. Further embodiments may have different device, system, and method configurations to measure cells in a fluid sample using centrifugal forces and density media.

[0064] FIG. **9** is a schematic illustration of another embodiment of a cell quantification area **900** arranged in accordance with the present invention. The channel **225** may be coupled to the detection region **230** by a microfluidic channel **905**, which may have a dimension selected such that the microfluidic channel **905** may serve as a valve, allowing fluid flow into the detection area responsive to a threshold level of centrifugal force. A chamber **915** may be coupled to the detection area **230** and configured to contain a density media. Another chamber **910** may be coupled to the detection area **230** and configured to contain another density media. The density media in the chamber **915** may be less dense than the density media in the chamber **910**. So for example, the density media in the chamber **910** may have a density greater than a density of a fluid sample but less than a density of one cell type in the fluid sample. The density media in the chamber **915** may have a density greater than a density of a fluid sample, but less than the density media in the chamber **910** and less than a density of another cell type in the fluid sample. As will be described further below, the density media may be placed adjacent one another in the detection area **230**, and cells in a fluid sample may be drawn through the density media to the interface between the density media.

[0065] FIG. **10** is a flowchart illustrating an example method for measuring cells according to an embodiment of the present invention. Prior to block **1005**, one or more of the sample preparation steps, such as those described above with reference to blocks **410** and **415** of FIG. **4**, may be performed. In block **1005**, density media and a fluid sample may be layered in a detection region. Block **1005** may be followed by block **1010** in which cells may be separated from the fluid sample by drawing the cells through the layered density media. Block **1010** may be followed by block **1015**. In block **1015**, signal may be detected from label moieties affixed to cells at an interface of at least one of the density media in the detection region.

[0066] In block **1005**, density media and a fluid sample may be layered in a detection region. As has been described above, multiple density media may be used, including two density medias having different densities. The density media and fluid sample may be layered in a single step, or the density medias may be layered first, followed by the fluid sample. Layering may be achieved by transporting individual ones of the density media and fluid sample sequentially into the detection region. In other examples, layering may be achieved by spinning a microfluidic disk such that the density media and fluid sample are transported into the detection region.

[0067] FIG. **11** is a schematic illustration of a portion of the cell quantification region **900** of FIG. **9** showing a density media loaded into the chamber **910**, another density media loaded into the chamber **915**, and a fluid sample loaded in the channel **225**. The microfluidic disk may then be spun to generate a centrifugal force to cause the density medias and the fluid sample to enter the detection region **230**. The density media in the chamber **910** may be denser than the density media in the chamber **915**, which may in turn be denser than the fluid sample in the channel **225**. In one example, the density media in the chamber **910** may have a density 1.091,

which may be implemented using a 70% Percoll concentration, while the density media in the chamber **915** may have a density of 1.078, which may be implemented using a 60% Percoll concentration. Other densities and concentrations may also be used.

[0068] FIG. **12** is a schematic illustration of the portion of the cell quantification area **900** of FIG. **11** following layering. The density media from the chamber **910** has been transported to a peripheral region of the detection region **230**, followed by the density media from the chamber **915**, and the fluid sample from the channel **225**. In one embodiment, the layering process included spinning a microfluidic disk at 1000 RPM for thirty seconds. The time and speed selected will vary based on the channel and chamber dimensions and fluids involved.

[0069] In block **1010**, cells may be separated from the fluid sample by drawing the cells through the layered density media using a centrifugal force. As has been described above, block **1010** may be implemented by spinning a microfluidic disk. Components of the fluid sample denser than both density media may be drawn toward the far peripheral portion of the detection region. Components of the fluid sample denser than one density media, but less dense than another may separate to a location at the interface between the density medias. Components of the fluid sample which are less dense than both density media may remain above both density media.

[0070] FIG. **13** is a schematic illustration of the portion of cell quantification region **900** of FIG. **12** following cell separation of a whole blood sample. Unlysed red blood cells, if present, may be transported to a peripheral location **1305** of the detection region. Granulocytes may be separated at a band **1310** located at an interface between the two density medias. The granulocytes may be less dense than the density media from the chamber **910**, but more dense than the density media from the chamber **915**. Monocytes and lymphocytes may be separated together at a band **1315**, and may not be separated from one another, as both may be less dense than the density media from the chamber **915**.

[0071] As generally described above, a detection module may be positioned to detect one or more of the bands **1305**, **1310**, and **1315**. The detection module may include an actuator, as shown in FIG. **3**, to move a detector along the detection region and detect signal from each of the bands. The signal peaks detected at particular distances may be integrated to quantify a relative count of cells pertaining to each density range. In some cell count application which utilize relative granulocyte count, such as radiation biodosimetry or sepsis, this embodiment may be advantageous since the granulocytes are separated from remaining components.

[0072] Examples of the separation and quantification of particles in a sample fluid have accordingly been described above. In some examples, a separated component of a sample fluid may be subject to one or more post-processing procedures. FIG. **14** is a schematic illustration of a portion of a cell quantification area **1405** including a post-processing area **1410**. The cell quantification area **1405** is shown including components shown and described above with reference to FIG. **7**, and like reference numbers are retained. The detection region, however, may be coupled to a post-processing area **1410** by a channel **1430**. Access between the detection region and the post-processing area **1410** may be controlled by a valve **1420**. By selecting a time at which the valve **1420** is opened, the components diverted to the post-processing area

1410 may be selected. That is, as components sediment out of a fluid sample and travel toward an end of the detection region, they may be diverted toward the post-processing area **1410** once the valve **1420** is opened. Accordingly, particles may be diverted to the post-processing area **1410** prior to complete sedimentation of all particles.

[0073] The post-processing area **1410** may be a channel, chamber, and/or reservoir of substantially any shape or size and may be partially defined by a same substrate as the detection region. Any of a variety of post-processing procedures or treatments may occur in the post-processing area **1410** included, but not limited to lysis, PCR, immunoassay, and/or biochemical analysis. In other examples, no post-processing procedures may occur, but a particular component of the sample may be stored in the post-processing area **1410**.

[0074] In some examples, bacteria and/or viruses may be separated from a fluid sample. Bacteria and/or viruses are generally smaller than mammalian cells, and may accordingly sediment much more slowly or not at all through a density media during centrifugation. In some examples, bacteria and/or viruses may be labeled and quantified in an analogous manner to that described above for particles to quantify infection load in a fluid sample. The smaller particles such as the bacteria and/or viruses may generally be detected at or near a top of the density media. Referring to FIG. **14**, the bacteria and/or viruses may be diverted to the post-processing area **1410** by opening the valve **1420**. Centrifugation may divert the bacteria and/or viruses to the post-processing area **1410**. Further processing such as lysis, PCR, immunoassay, or harvesting of the contents of the post-processing area **1410** for subsequent culture may be performed to identify bacteria and/or viruses.

[0075] As another example, the valve **1420** of FIG. **14** may be opened during centrifugation at a time when lymphocytes are expected to be above the intersection of the channel **1430** and the detection region **230**. The lymphocytes may then be diverted to the post-processing area **1410**. Additional analysis of the separated lymphocytes may then be performed, such as PCR for gene expression analysis.

[0076] As another example, tumor cells, which may be denser than other components of a fluid sample, may be separated, counted, and analyzed from a biopsy homogenate by removing the smaller cells through the channel **1430**. More generally, a particular cell population may be selected from a mixture of components in a fluid sample for further biochemical analysis based on the differential size and density of the cell population. The cell population diverted to the post-processing area **1410** may also be counted or quantified in the post-processing area **1410** using methods described above.

[0077] From the foregoing it will be appreciated that, although specific embodiments of the invention have been described herein for purposes of illustration, various modifications may be made without deviating from the spirit and scope of the invention.

What is claimed is:

1. An apparatus for measuring a quantity of particles in a fluid sample, the apparatus comprising:
 - a substrate, wherein the substrate at least in part defines a channel;
 - an inlet port in fluid communication with the channel and configured to receive the fluid sample;
 - a detection region coupled to the channel and defined at least in part by the substrate and configured to contain a

density media, wherein the density media has a density lower than a density of the particles and higher than a density of the fluid sample; and

wherein the channel and the detection region are configured to transport the quantity of particles in the fluid sample from the channel through the density media responsive to a centrifugal force, and wherein at least a portion of the fluid sample is restricted from transport through the density media.

2. The apparatus of claim 1, wherein the substrate comprises a disc.

3. The apparatus of claim 1, further comprising a media reservoir defined at least in part by the substrate and in fluid communication with the detection region, wherein the media reservoir and the detection region are configured such that the density media is transported from the media reservoir to the detection region responsive to a centrifugal force.

4. The apparatus of claim 1, further comprising a label reservoir in fluid communication with the channel, wherein the label reservoir is configured to contain label moieties, and wherein the label moieties are configured to label the quantity of particles.

5. The apparatus of claim 1, wherein the density media comprises a plurality of density medias, and wherein the channel and detection region are further configured to transport the quantity of particles to an interface between the plurality of density medias responsive to a centrifugal force.

6. A system for measuring a quantity of particles in a fluid, the system comprising:

a disk comprising:

a substrate, wherein the substrate at least in part defines a channel;

an inlet port in fluid communication with the channel and configured to receive the fluid;

a detection region coupled to the channel and defined at least in part by the substrate and configured to contain a density media, wherein the density media has a density lower than a density of the particles and higher than a density of the fluid sample; and

wherein the channel and detection region are configured to transport the quantity of particles in the fluid sample from the channel through the density media

responsive to a centrifugal force, and wherein at least a portion of the fluid sample is restricted from transport through the density media;

a motor coupled to the disk, the motor configured to receive a motor control signal and spin the disk responsive to the motor control signal;

a detection module positioned to detect a signal from label moieties affixed to the quantity of particles, wherein the detection module is configured to generate an electronic detection signal based, at least in part, on the signal from the label moieties; and

a processing device coupled to the motor and the detection module, wherein the processing device is configured to generate the motor control signal and provide the motor control signal to the motor, and wherein the processing device is further configured to receive the electronic detection signal from the detection module.

7. The system of claim 6, wherein the signal from the label moieties comprises an optical signal and wherein the detection module comprises a laser.

8. The system of claim 7, wherein the detection module further comprises an actuator coupled to the laser and the processing device, and wherein the actuator is configured to move the laser along the detection region responsive to an actuator control signal received from the processing device.

9. The system of claim 7, wherein the system further comprises an actuator coupled to the motor, and wherein the actuator is configured to move the disk such that the laser is moved along the detection region responsive to an actuator control signal received from the processing device.

10. The system of claim 7, wherein the processing device is further configured to calculate a number of the quantity of particles based, at least in part, on the electronic detection signal.

11. The system of claim 10, wherein the processing device is configured to integrate at least a portion of the electronic detection signal over time to calculate the number of the quantity of particles.

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