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(54) **BIOSIGNAL MEASUREMENT APPARATUS**

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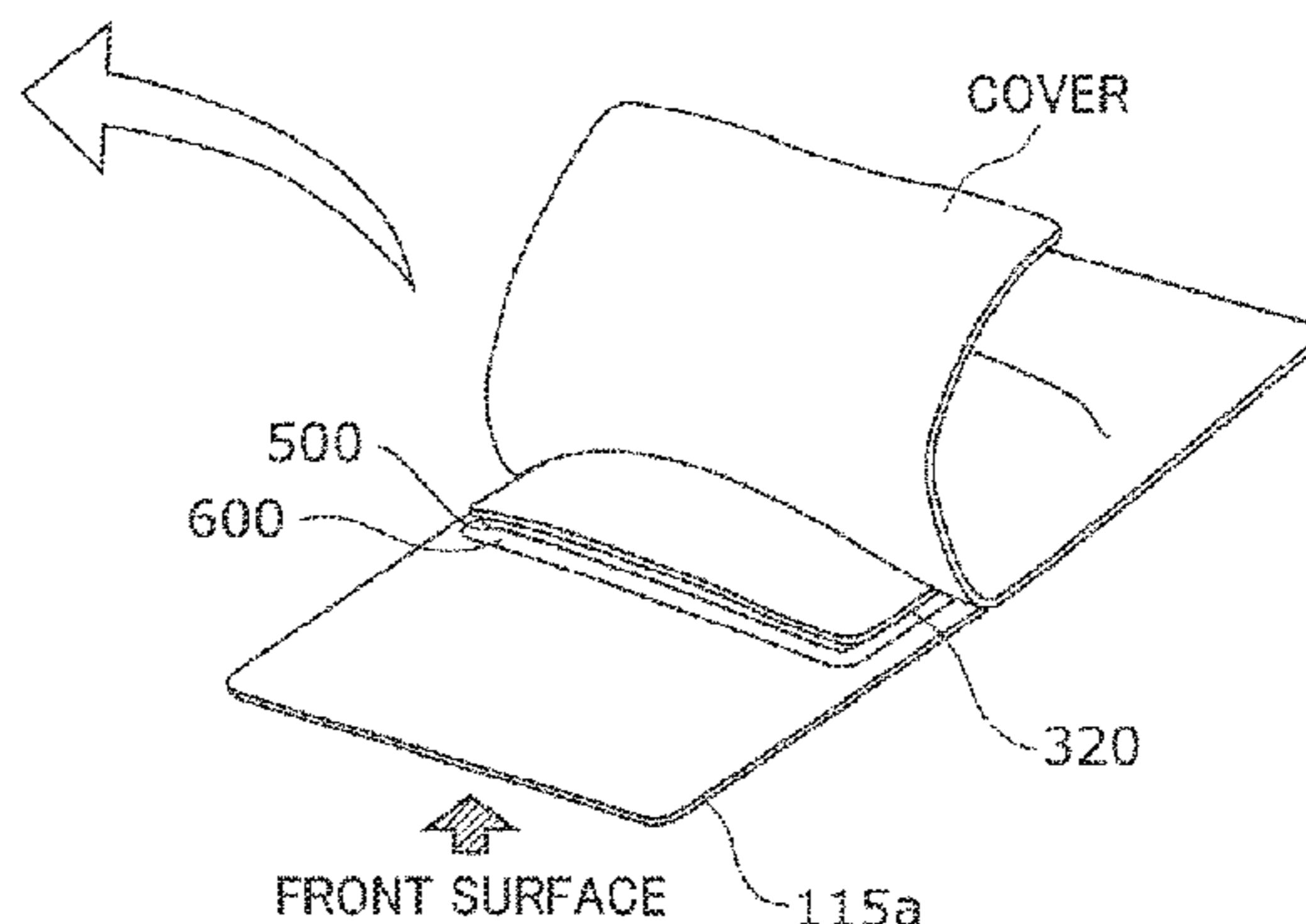
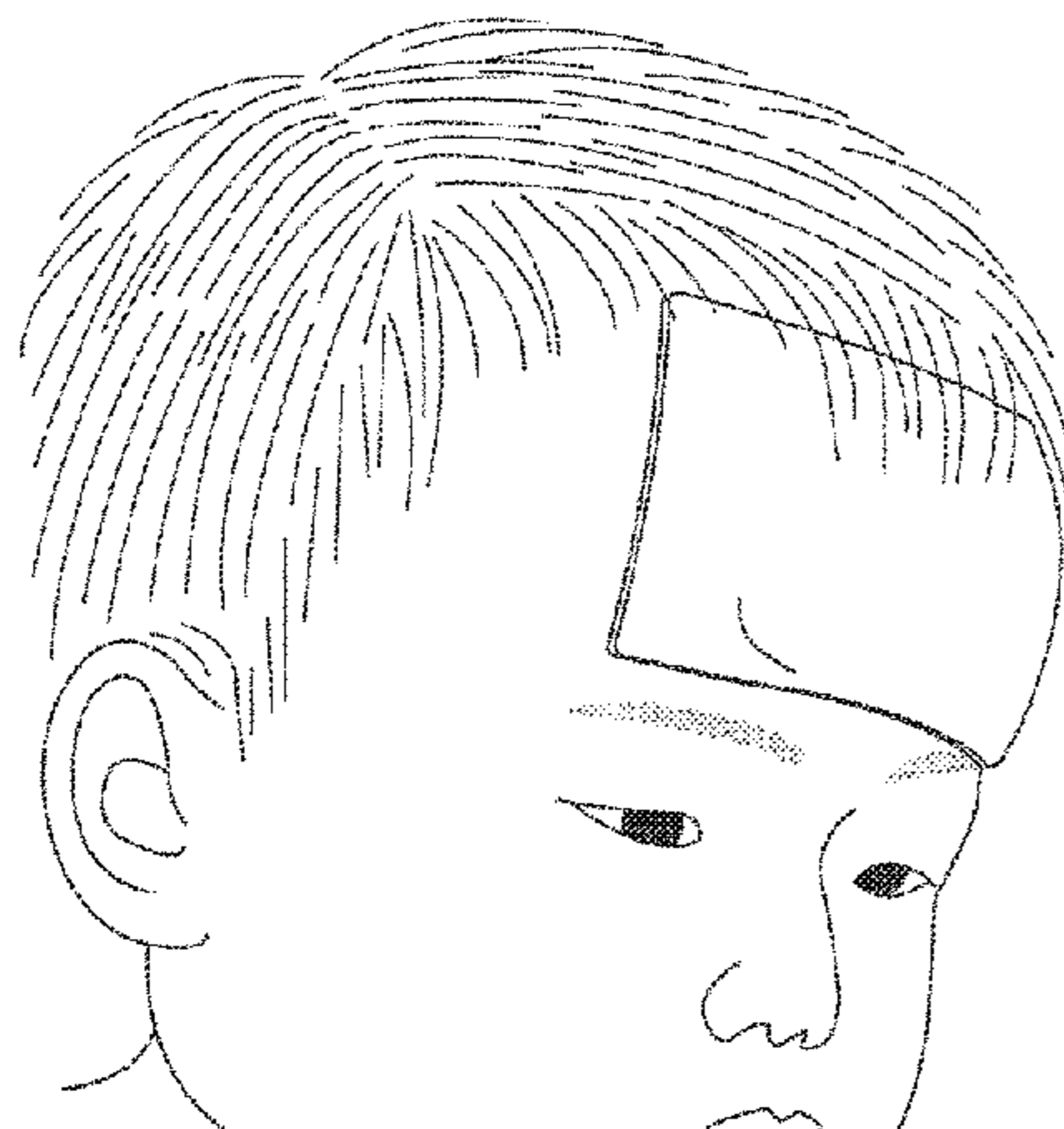
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(57) **ABSTRACT**

A biosignal measurement apparatus is used by being affixed on a living body. The apparatus includes an affixed part that is a sheet, in which a signal-acquiring section of multiple electrodes and wiring connected to each of the electrodes are formed, and which can be freely expanded, contracted and bent and is adhesive; and a substrate that is connected to the wiring and on which a signal-processing circuit for wirelessly transmitting biosignals obtained through the wiring is mounted. The signal-acquiring section is exposed on the surface of the affixed part and the affixed part and the substrate are stacked so that the back surface of the affixed part faces the substrate.

**12 Claims, 6 Drawing Sheets**



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See application file for complete search history.

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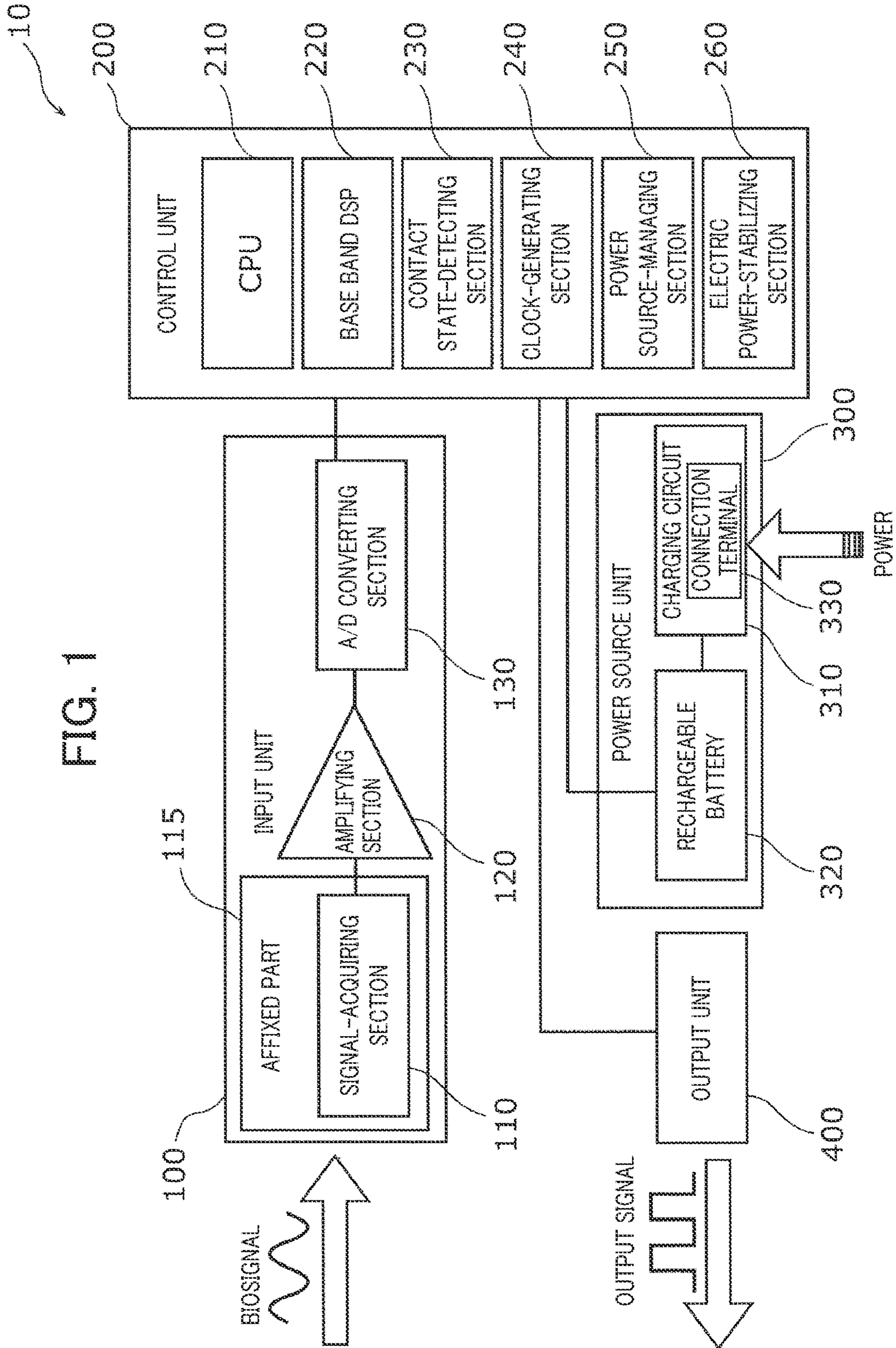
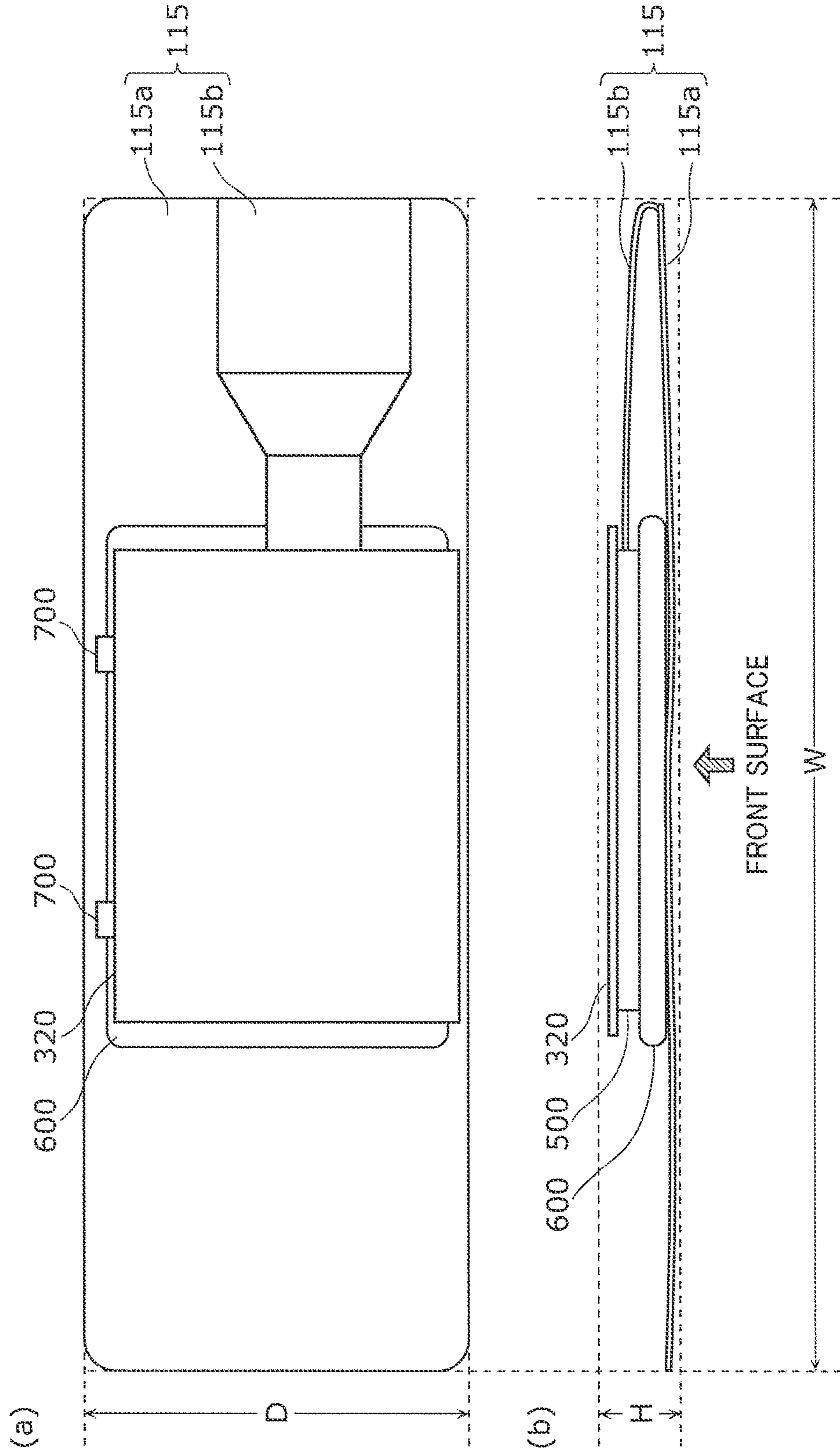


FIG. 1

FIG. 2



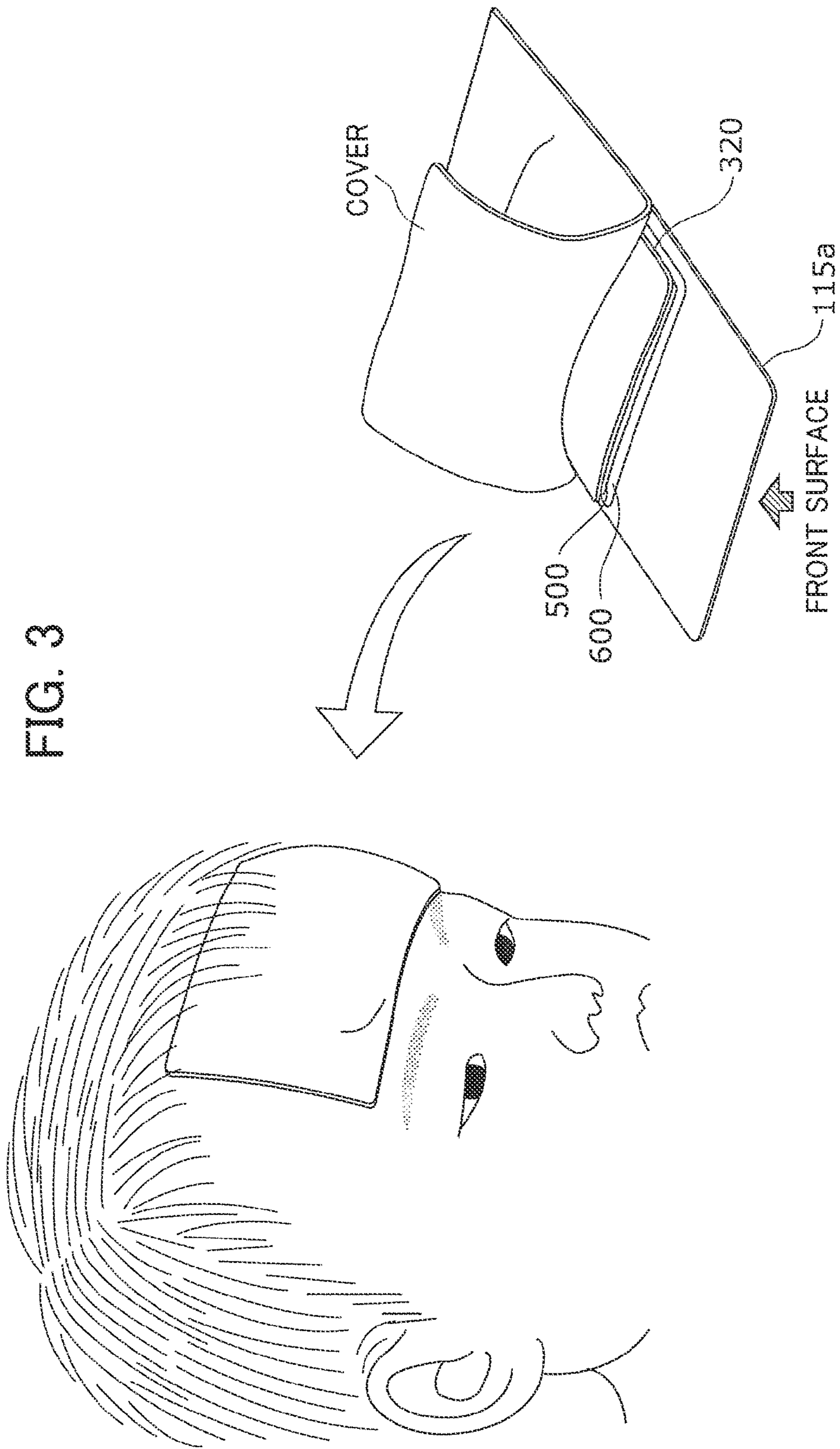




FIG. 4

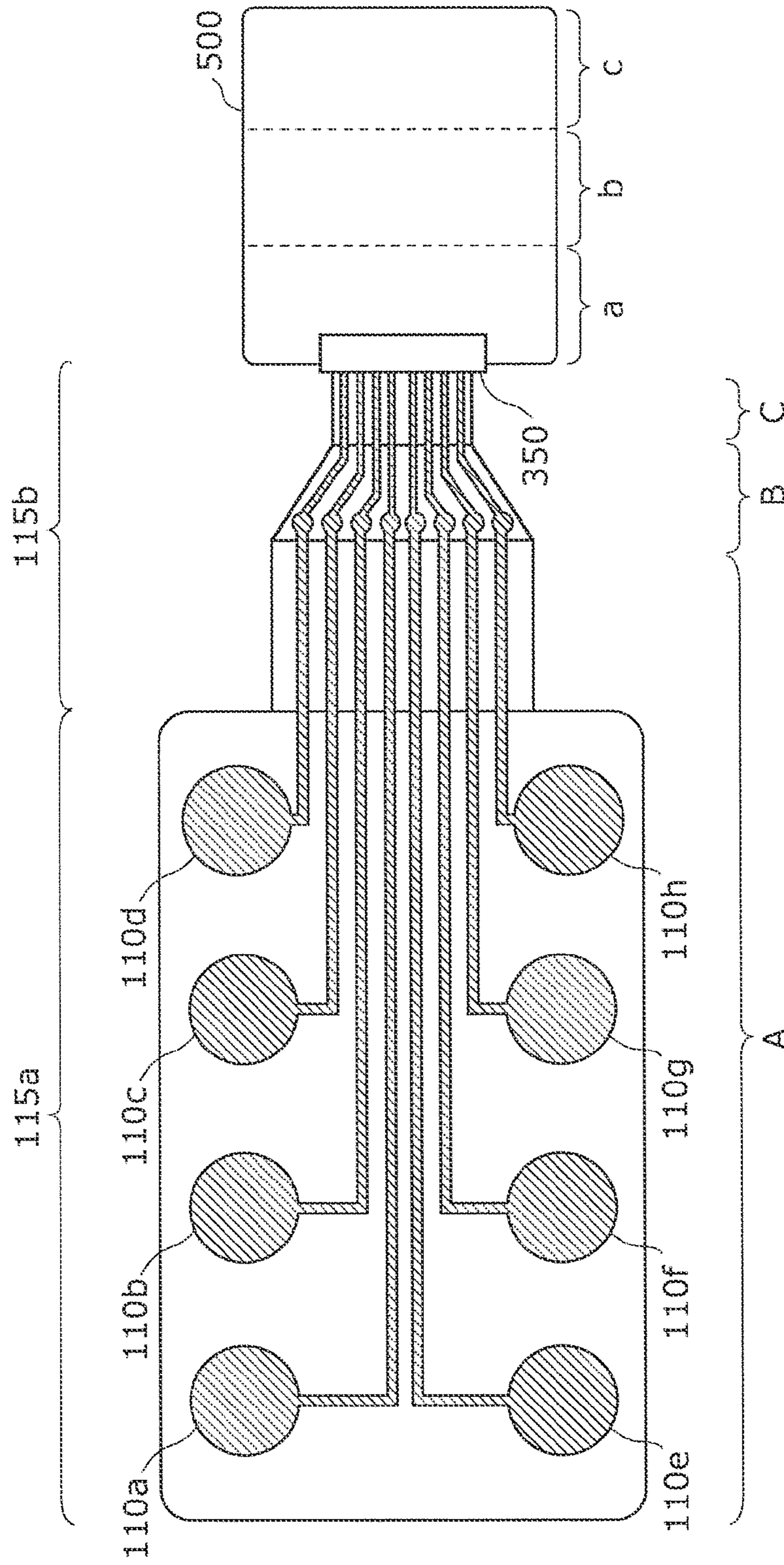


FIG. 5

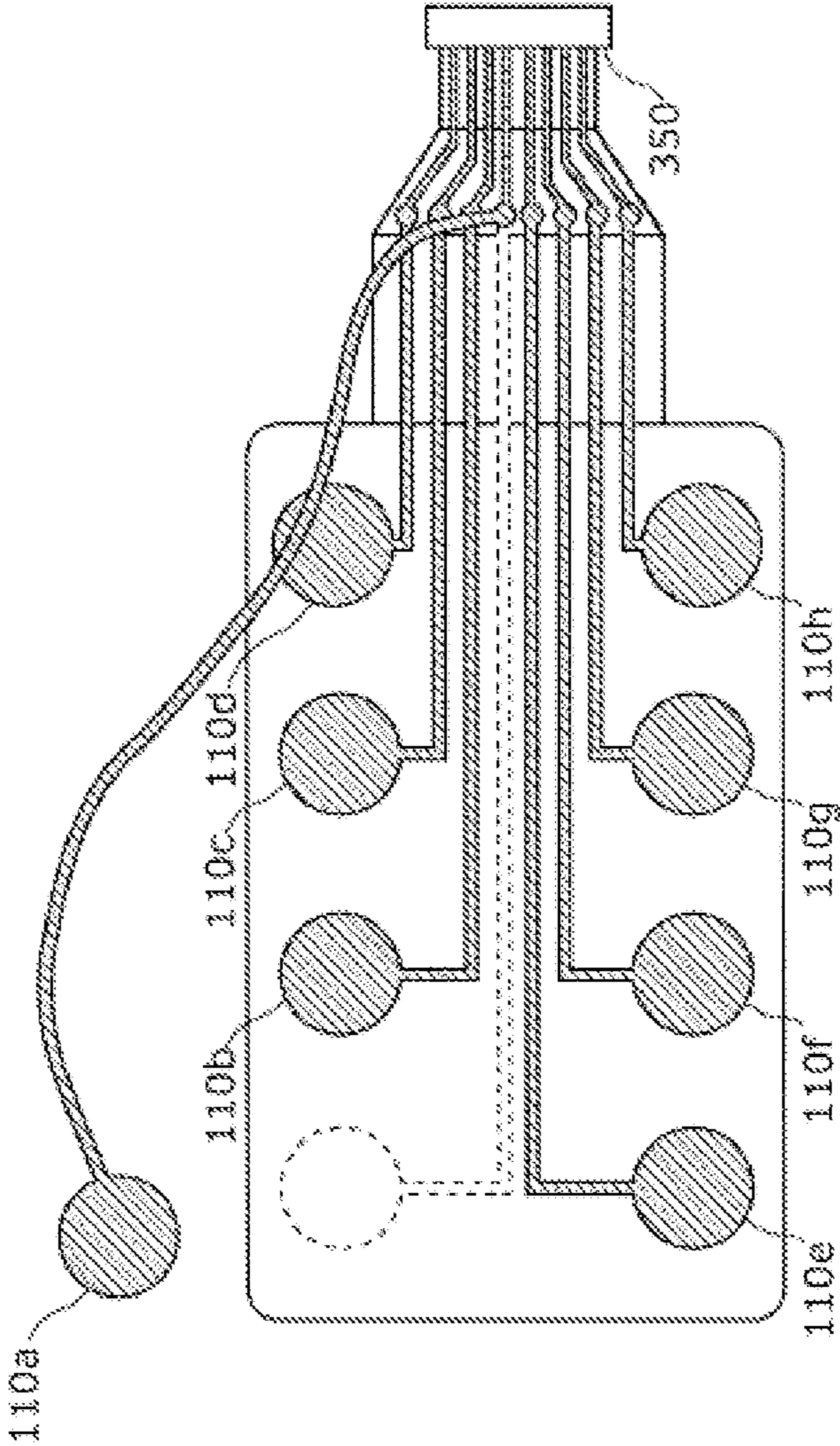




FIG. 6A

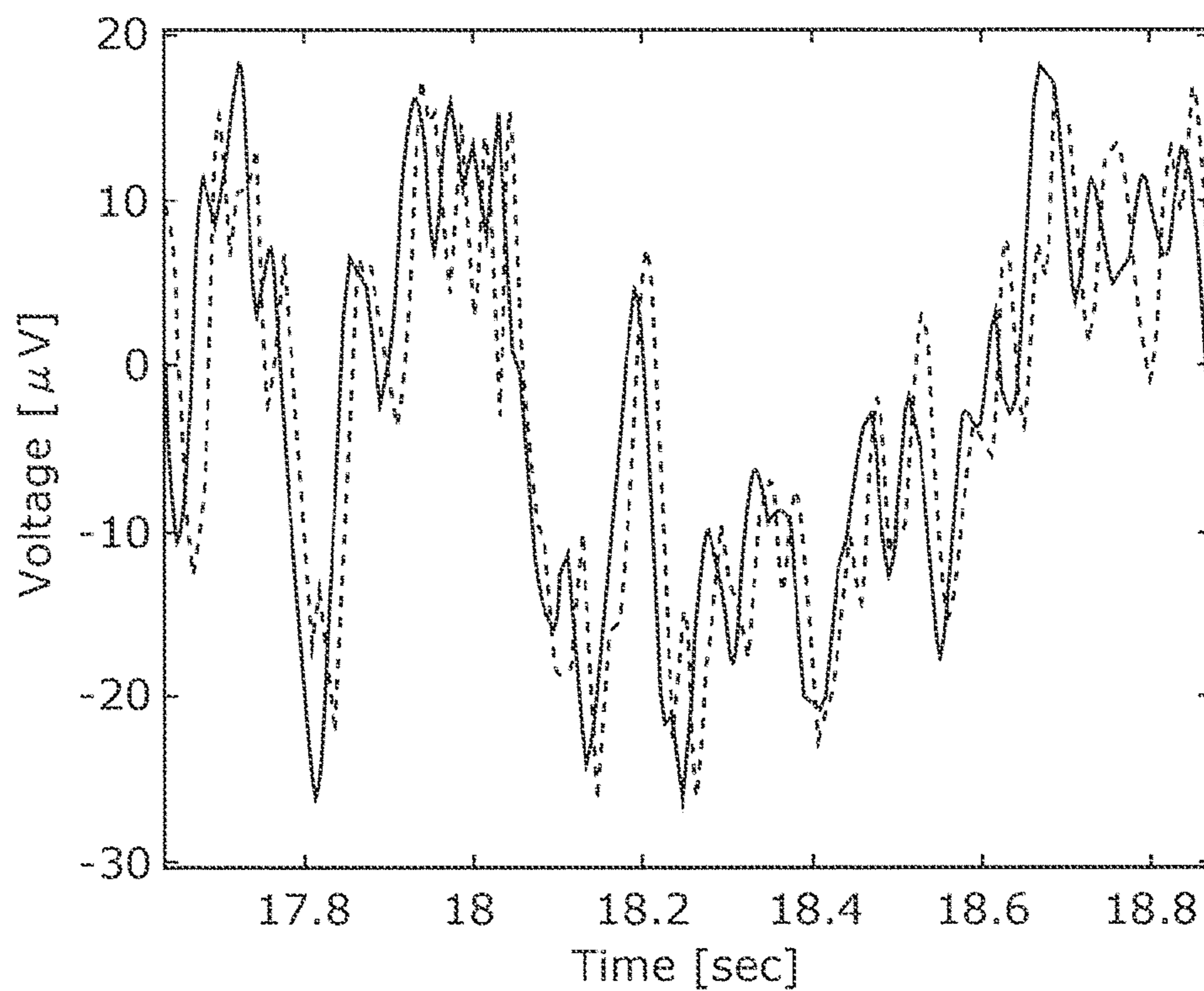
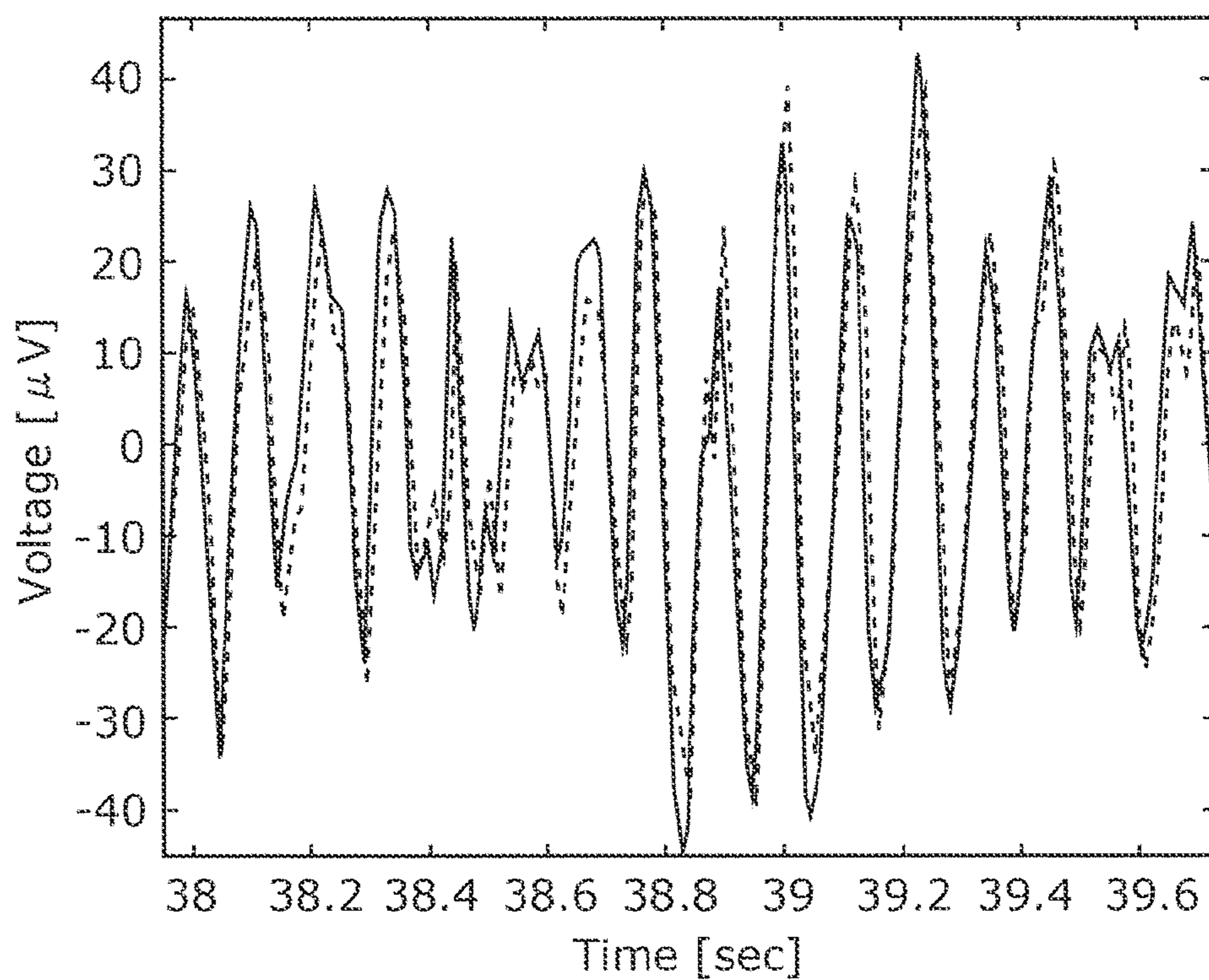


FIG. 6B





**BIOSIGNAL MEASUREMENT APPARATUS**INCORPORATION BY REFERENCE TO ANY  
PRIORITY APPLICATIONS

Any and all applications for which a foreign or domestic priority claim is identified in the Application Data Sheet as filed with the present application are hereby incorporated by reference under 37 CFR 1.57.

## BACKGROUND OF THE INVENTION

## Field of the Invention

The present invention relates to an apparatus for measuring a potential variation with time with an electrode, such as electrical activity in a living body.

## Description of the Related Art

The potential variation generated accompanying activity in a living body, such as brain waves and an electrocardiogram, is measurable via an electrode attached to the outside of the living body. In a hospital, a research institute and the like, the potential variation measured in such a manner is conventionally used as a biosignal to noninvasively grasp the presence or absence of abnormality and the degree thereof in a living body. An apparatus for the measurement, that is, an examination instrument for medical use or for research use such as an electroencephalograph or an electrocardiograph, is downsized as with consumer apparatus. Such an examination instrument is required to have high precision, and is used in a consultation room or an examination room of medical facilities, a visit destination or the like to a subject who is in a state of low activity, in many cases. Therefore, even a downsized examination instrument, for example, an electroencephalograph, is formed to have such a size and weight as to have portability to the extent of being movable when the instrument not in use is set on a base with a caster or stored in a dedicated case (refer to Non-Patent Document 1).

On the other hand, a portable size electrocardiograph is available, and is configured with a main body of a rigid housing, and a plurality of cables each which extends from the main body or is connected to the main body, and which has an electrode at the tip thereof (refer to Non-Patent Document 2).

## Non-Patent Document 1

Physiological examination equipment: electroencephalograph, produced by Nihon Kohden Corporation, [online] Dec. 8, 2015, [Searched on Jan. 5, 2016], Website (URL: [http://www.nihonkohden.co.jp/iryoo/products/physio/03\\_eeg/index.html](http://www.nihonkohden.co.jp/iryoo/products/physio/03_eeg/index.html))

## Non-Patent Document 2

Physiological examination equipment: electrocardiograph, produced by Nihon Kohden Corporation, [online] Dec. 25, 2015 [Searched on Jan. 5, 2016], Website (URL: [http://www.nihonkohden.co.jp/iryoo/products/physio/01\\_ecg/index.html](http://www.nihonkohden.co.jp/iryoo/products/physio/01_ecg/index.html))

## SUMMARY OF THE INVENTION

## Problems to be Solved by the Invention

Examination by a conventional examination instrument gives not much physical burden on a subject, if the exami-

nation is carried out for a relatively short period of time at a specific place as described above. However, the burden may be inappropriately large in some cases depending on the purpose of an examination or on a subject.

As a specific example, an examination for acquiring a biosignal during sleep is considered below. A plurality of electrodes to be worn, an application agent applied at a portion on which the electrodes are worn, contact to the skin of the cables connecting the electrodes and the main body, and the like impart strong wearing feeling or uncomfortable feeling to a subject to disturb the onset of sleep of the subject, or affect electrical activity occurring in the subject's body. As a result, biosignal of the subject during normal sleep is not acquired. It may be difficult to perform the examination, especially in some cases where a subject who has a low anti-stress property such as an infant or a young child or a subject who has insufficient control ability of the body show large body response against the wearing feeling and/or the uncomfortable feeling.

A conventional electroencephalograph restricts the motion of a subject by the cables, whereby the situations where measurement can be performed are limited. In an example, monitoring with measurement is not available with respect to a biosignal of a subject who takes daily action.

Furthermore, the examination by the examination instrument as described above is performed in a relatively large scale. The measurement of brain waves is basically difficult to be performed by a patient or patient's family member at home, unlike a simple examination with a stethoscope, a sphygmomanometer, a clinical thermometer or the like, and thus needs to be performed in medical facilities. A portable electrocardiograph is usable at home, but is limited in performance such as due to the number of channels. Therefore, a biosignal of a patient even not in a serious situation may need to be measured in medical facilities, thereby requiring not only the physical burden on the patient (subject) described above, but also a time burden and a financial burden on both of the subject and the medical facilities.

The present invention has been made in view of these problems. The object of the present invention is to provide a biosignal measurement apparatus for combining ease of measurement and high performance with less wearing feeling and less uncomfortable feeling imparted to a subject.

## Means for Solving the Problems

The biosignal measurement apparatus according to the present invention, which is provided to achieve the above-described object, is a biosignal measurement apparatus to be used by being affixed on a living body. The biosignal measurement apparatus includes a sheet which is formed with a plurality of electrodes and a plurality of wirings connected to the plurality of electrodes respectively, and which is freely expanded, contracted and bent, and is adhesive, and a substrate which is connected to the plurality of wirings and equipped with a signal processing circuit for wirelessly transmitting a biosignal acquired via the plurality of wirings. The plurality of electrodes are exposed on a front surface of the sheet, and the sheet and the substrate are stacked so that a back surface of the sheet faces the substrate.

The plurality of electrodes included in the biosignal measurement apparatus are affixed together with the sheet which is affixable like a poultice, on the living body. Therefore, an application agent is not required, and no cable is in contact with the skin. Since the affixed sheet and the electrodes follow the shape and motion of the affixed portion of the living body, the sheet and the electrodes are hardly



displaced and hardly peel off from the affixed portion. The biosignal measurement apparatus is configured so that the substrate and the sheet are stacked to be compactly assembled as a whole, and has no cable restricting the motion of the subject, thereby hardly imparting wearing feeling and uncomfortable feeling to the subject.

In such a biosignal measurement apparatus, each of the sheet and the substrate under the state of the front surface of the sheet affixed on the living body may have an outer shape in plan view of a size falling within a rectangle of 5 cm×15 cm.

This provides the biosignal measurement apparatus which has the entire size falling within the forehead of a subject and is capable of measuring the brain waves of the subject.

The plurality of electrodes may include a reference electrode and a plurality of measurement electrodes.

This allows measurement of a potential variation based on a reference potential acquired within the range of the affixed portion, as a biosignal with multiple channels.

The reference electrode may be affixed on the sheet in an aspect of being attachable to and detachable from the sheet.

This allows, for example, a medical staff member to use the biosignal measurement apparatus to carry out the measurement method based on the same principle as that of the biosignal measurement method which has been conventionally carried out. Therefore, the medical staff member feels less operation resistance to this biosignal measurement apparatus even if the shape and size are different from those of a conventional apparatus. The biosignal acquired by use of the biosignal measurement apparatus is used with the same feeling as the signal acquired by a conventional apparatus.

The plurality of electrodes may include some electrodes arranged parallelly in at least two rows, and each of the rows may include a plurality of electrodes in line.

This allows the biosignal to be continuously measured at the affixed portion, even if some of the electrodes are peeled off from the skin.

The sheet may have a flexible connecting part. The plurality of wirings may extend respectively and correspondingly from the electrodes to the connecting part. The connecting part may be bent so that the sheet is folded back, and a tip of the connecting part may be connected to the signal processing circuit.

This allows the substrate including the signal processing circuit and the sheet including the electrodes and the wirings to be arranged so as to be folded back and stacked, thereby enabling to provide the entire biosignal measurement apparatus in a smaller size in plan view.

The connecting part of the sheet may be configured so as to increase in hardness from a portion close to the plurality of electrodes toward a portion close to the tip.

This prevents stress from concentrating at the tip portion of the sheet connected to the substrate, thereby enabling to prolong the service life of the sheet.

The signal processing circuit may include an analog circuit for processing an analog signal acquired via the plurality of electrodes to convert the analog signal into a digital signal, a digital circuit for processing the digital signal acquired by the analog circuit to transmit the digital signal wirelessly, and a power source circuit for supplying power to the analog circuit and the digital circuit. The analog circuit, the digital circuit and the power source circuit may be respectively mounted in a first region, a second region and a third region obtained by dividing a mounting surface of the substrate into three regions.

This suppresses noise coming in between the analog circuit and the digital circuit.

The analog circuit may have an A/D converting section for converting the analog signal into a digital signal having a bit number of 20 bits or more.

This allows measurement with high resolution comparable to a conventional biosignal measurement apparatus.

The analog circuit may have a contact state-detecting circuit for detecting a contact state between the plurality of electrodes and the living body by measuring a contact impedance between the plurality of electrodes and the living body.

This makes it possible to confirm the contact state between the electrodes and the skin of the subject, thereby ensuring and maintaining the wearing state in which appropriate measurement is available.

The power source circuit may include a rechargeable battery, a connection terminal provided on the substrate, and a charging circuit for charging the battery with power supplied through the connection terminal.

This allows the biosignal measurement apparatus to be used as a wearable measurement apparatus worn by the subject.

It is noted that the generic or specific aspects may be realized by a system, an integrated circuit, a computer program, or a recording medium such as a computer-readable CD-ROM, or may be realized by an arbitrary combination among a system, an integrated circuit, a computer program and a recording medium.

#### Effects of the Invention

The present invention provides a biosignal measurement apparatus for combining ease of measurement and precision with less wearing feeling and less uncomfortable feeling imparted to a subject.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram illustrating the outline of the configuration of a biosignal measurement apparatus according to an embodiment of the present invention.

FIG. 2 is a schematic diagram illustrating the appearance of the configuration of the biosignal measurement apparatus used as an electroencephalograph according to an example of the present invention.

FIG. 3 is a diagram illustrating an example in which a subject wears the biosignal measurement apparatus according to the example of the present invention.

FIG. 4 is a diagram illustrating a configuration example of an affixed part including a signal-acquiring section and a substrate, of the biosignal measurement apparatus according to the example of the present invention.

FIG. 5 is a diagram illustrating another configuration example of the affixed part including the signal-acquiring section and the substrate, of the biosignal measurement apparatus according to the example of the present invention.

FIG. 6A is a diagram for comparing the brain waves measured by the biosignal measurement apparatus according to the example of the present invention and the brain waves measured by a brain wave measuring apparatus for medical use at the same time.

FIG. 6B is another diagram for comparing the brain waves measured by the biosignal measurement apparatus according to the example of the present invention and the brain



waves measured by a brain wave measuring apparatus for medical use at the same time.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

Some embodiments will be specifically described below with reference to the drawings.

It is noted that each of the embodiments described below represents a comprehensive or specific example. Numerical values, shapes, materials, constituent elements, arrangement positions and connection configurations of the constituent elements, and the like indicated in the following embodiments are mere examples, not intended to limit the present invention. Among the constituent elements in the following embodiments, the constituent elements not described in the independent claims each meaning the highest order concept are described as arbitrary constituent elements.

#### Embodiment

##### [1. Overall Configuration]

FIG. 1 is a block diagram illustrating the outline of the configuration of a biosignal measurement apparatus 10 according to the present embodiment.

The biosignal measurement apparatus 10 is an apparatus for measuring a potential variation with time occurring in a living body with an electrode to acquire it as a biosignal, and outputting data on the biosignal. The potential variation in a living body herein is the minute potential variation (several tens of microvolts to several tens of millivolts) occurring by the activity of, for example, brain, heart or other muscle.

The biosignal measurement apparatus 10 includes an input unit 100, a control unit 200, a power source unit 300, and an output unit 400. The physical arrangement of these constituent elements will be described below by use of examples.

The input unit 100 measures a detectable potential in a living body via the skin of the living body, and outputs a signal indicating a time series variation of the measured potential to the control unit 200. The input unit 100 includes a signal-acquiring section 110, an affixed part 115, an amplifying section 120, and an analog-to-digital converting section (hereinafter and in FIG. 1, also referred to as an A/D converting section) 130.

The signal-acquiring section 110, which is of multiple thin film electrodes, is formed so as to be exposed on one surface of the affixed part 115 which is an adhesive sheet. In the following description, the surface side of the affixed part 115 on which the signal-acquiring section 110 is exposed is also referred to as the front surface of the affixed part 115, while the opposite surface is also referred to as the back surface. The affixed part 115 is affixed on a living body such that the front surface thereof comes into contact with the skin of the living body. The signal-acquiring section 110 detects a potential under such a state. The potential of each of the multiple electrodes of the signal-acquiring section 110 is measurable. The biosignal acquired by measuring the potential with each of the electrodes is input to the control unit 200 via the amplifying section 120 and the A/D converting section 130 through an individual transmission path (channel). It is noted that these electrodes include one or more reference electrodes and one or more measurement electrodes, and the biosignal is acquired in such a manner that the potential difference between each measurement electrode and the reference electrode corresponding to the measurement electrode is measured.

Each of the signal-acquiring section 110 and the affixed part 115 has expandability and contractibility, and flexibility allowing free bending, and thus follows, when affixed on the body surface of a subject, the shape and motion of the affixed portion thereof.

As an example, an adhesive base material is used as the affixed part 115 having such characteristics, made of a silicone material for use as a base material such as of a poultice. The affixed part 115 made of such material has high moisture permeability in addition to high expandability and contractibility and high flexibility, thereby enabling to suppress the subject from feeling uncomfortable and sweating during wearing. Such material also has high biocompatibility, whereby the affixed part 115 is capable of being worn for a long period.

The signal-acquiring section 110 of multiple electrodes may be made of an expandable and contractible conductor using metal particles. In addition, wiring, which is formed on the affixed part 115 so as to transmit a signal from the signal-acquiring section 110 to the outside of the affixed part 115, may be made of the expandable and contractible conductor. The electrodes and wiring made of the expandable and contractible conductor are capable of expanding up to approx. 700%. Silver nanowire, for example, may serve as the metal particles, whereby a conductivity of approx. 10000 S/cm is acquired. Accordingly, the biosignal of a subject is input to the amplifying section 120 described below through the electrodes and wiring having low resistance and low noise. That is, each of the signal-acquiring section 110 and the wiring, which are made of the expandable and contractible conductor, combines expandability and contractibility, preferable transparency, and conductivity, and its expandability disturbs no motion of a subject.

The affixed part 115 on which the signal-acquiring section 110 and wiring are formed is a sheet which is freely expanded, contracted and bent as a whole and is adhesive, and which is capable of being worn for a long period.

It is noted that in the signal-acquiring section 110, the expandable and contractible conductor made of metal particles may not be exposed on the front surface of the affixed part 115. In an example, the signal-acquiring section 110 may be configured with a conductive gel material and the expandable and contractible conductor stacked in layers, wherein the gel material may be exposed on the front surface of the affixed part 115, while the expandable and contractible conductor may be embedded in the affixed part 115. This suppresses the deterioration of the expandable and contractible conductor caused by oxidation of metal particles or the like, and also makes the biosignal measurement apparatus 10 according to the present embodiment available even to a subject having allergy to metal.

The amplifying section 120 amplifies the biosignal input by the signal-acquiring section 110, and outputs the signal to the A/D converting section 130. The amplifying section 120 may be realized as, for example, an amplifying circuit including an operational amplifier on a substrate described below.

The A/D converting section 130 converts into a digital signal the biosignal which is an analog signal input by the amplifying section 120, and outputs the signal to the control unit 200. It is noted that in order to obtain precision (resolution) comparable to that of a conventional medical instrument, the A/D converting section 130 of the biosignal measurement apparatus 10 according to the present embodiment is realized by an A/D converting section for converting



an analog signal into a digital signal having a bit number of 20 bits or more. For example, a 24-bit  $\Delta\Sigma$  type A/D converter is used.

The control unit **200** controls the entire operation of the biosignal measurement apparatus **10**. The control unit **200** includes a central processing unit (hereinafter also referred to as CPU, and indicated as CPU in FIG. 1) **210**, a base band digital signal processor (hereinafter also referred to as a base band DSP, and indicated as DSP in FIG. 1) **220**, a contact state-detecting section **230**, a clock-generating section **240**, a power source-managing section **250**, and an electric power-stabilizing section **260**.

The CPU **210** reads out and executes a program from a storage section (not shown) to manage and control operation of each of the constituent elements included in the biosignal measurement apparatus **10**.

The base band DSP **220** performs predetermined processing on the digital signal input by the input unit **100**, and then outputs the digital signal to the outside via the output unit **400**.

The contact state-detecting section **230** is an electronic circuit (a contact state-detecting circuit) for detecting a contact state between the living body and the signal-acquiring section **110** of electrodes. Specifically, the contact state-detecting section **230** measures a contact impedance between the signal-acquiring section **110** and the skin of the living body, and determines whether the contact state is good or poor on the basis of the magnitude of the contact impedance. The determination is made during, for example, wearing and measurement of the biosignal, thereby ensuring the proper wearing state of the biosignal measurement apparatus **10**. It is noted that the criterion for determining that the contact state is poor may be changed as appropriate through setting. In the case where the input unit **100** has 8 channels of signal input paths, as an example, the contact state may be determined poor when even one channel of an electrode out of the eight channels is detected as being disconnected (in a lead-off state) from the subject. Alternatively, the contact state may be determined poor when a majority of five channels are detected each as being in a lead-off state.

The clock-generating section **240** is a clock generating circuit for generating an internal clock of the CPU **210**.

The power source-managing section **250** and the electric power-stabilizing section **260**, along with the power source unit **300** described below, constitute a power source circuit to supply the power input by the power source unit **300** as the power for driving the control unit **200** and other constituent elements. The power source-managing section **250** includes, for example, a DC-DC converter. The input unit **100** and the output unit **400** respectively receive power having different voltages transformed by the power source-managing section **250**. The electric power-stabilizing section **260** is a regulator for stabilizing the power for supplying.

The power source unit **300** supplies the power required for the operation of each of the constituent elements of the biosignal measurement apparatus **10** via the power source-managing section **250** and the electric power-stabilizing section **260** described above. The power source unit **300** includes a charging circuit **310** and a rechargeable battery **320**.

The charging circuit **310** is the circuit which, in order to charge the rechargeable battery **320**, receives power from the outside of the biosignal measurement apparatus **10** and controls the voltage and current of the received power, thereby supplying the controlled power to the rechargeable

battery **320**. The charging circuit **310** includes a connection terminal **330** for receiving power. The connection terminal **330** may be, for example, a power receiving terminal for receiving power from a commercial power outlet via a cable, or may be a port such as of a USB (universal serial bus) capable of receiving power from an external apparatus capable of supplying power.

The rechargeable battery **320** is a battery which is capable of being recharged and in which the power to be supplied to each of the constituent elements of the biosignal measurement apparatus **10** is stored. A battery having a capacity according to use application is used as the rechargeable battery **320**. In an example, the battery may have a capacity allowing continuous use for a long period of time enough for monitoring a subject in a wakeful state or a sleeping state. The rechargeable battery **320** is realized by, for example, a button type battery or a thin film battery, by taking into consideration the wearing feeling and the like imparted to the subject during use in addition to the capacity. This enables to suppress the increase in weight and size imparting stronger wearing feeling of the biosignal measurement apparatus **10**, and the decrease in followability to the shape of the living body.

The output unit **400**, which is a wireless communication module capable of wirelessly transmitting data, outputs in real time the biosignal output by the base band DSP **220** to an external apparatus of the biosignal measurement apparatus **10**, for example, a storage unit, a display unit such as a monitor, or an information terminal including these. A communication system based on a communication standard, for example, Bluetooth (registered trademark) or Wi-Fi (registered trademark) is used for the output unit **400** in the present embodiment. A low power consumption communication system such as Bluetooth (registered trademark) Low Energy (BLE) may be used, in order to prolong the continuous use period of time of the biosignal measurement apparatus **10**. It is noted that since each communication system has an upper limitation in an information amount (transmission rate) for real-time output according to its bandwidth, the sampling rate of the analog signal by the A/D converting section **130** is changed according to the communication system and the number of channels for measurement.

The biosignal measurement apparatus **10** according to the present embodiment having the above-described configuration is used in a manner that the affixed part **115** is affixed on a living body. When used as described above, the biosignal measurement apparatus **10** including the power source unit **300** and the output unit **400** described above are not required to have any power supply cable for constantly supplying power or any communication cable for constantly outputting biosignals. Accordingly, the subject wearing the biosignal measurement apparatus **10** feels no wearing feeling caused by these cables, and is not restricted in motion. Since the use of a plurality of electrodes provides the biosignal measurement apparatus **10** with redundancy, even if a lead-off state occurs due to motion or sweating of the subject, or the like, the biosignal measurement apparatus **10** is capable of monitoring the wearing state on the basis of the detection of the lead-off state. Accordingly, the use of the biosignal measurement apparatus **10** reliably ensures to execute monitoring even over a long period of time, as an example.

The biosignal measurement apparatus **10** having the above-described configuration is further capable of measuring a potential with high precision in a wide dynamic range with 24-bit measurement resolution. Specifically, the bio-



signal measurement apparatus **10** is capable of acquiring a minute biosignal of 1  $\mu\text{V}$  or less in the measurement range of  $\pm 2.5\text{V}$  with resolution of 0.2  $\mu\text{V}$ . The biosignal measurement apparatus **10** as described above has high versatility allowing application to measurement of brain waves, and various types of myoelectric potentials including a cardiac potential and an ocular potential.

[2. Example]

As described above, the biosignal measurement apparatus **10** having the above-described configuration is available as an electroencephalograph, an electrocardiograph, an electromyograph, and the like. The biosignal measurement apparatus **10** used as an electroencephalograph is specifically described below, taking it as an example of the biosignal measurement apparatus **10** according to the present embodiment.

[2-1. Overview]

FIG. **2** is a schematic diagram illustrating the appearance of the biosignal measurement apparatus **10** used as an electroencephalograph. FIG. **2(a)** is a plan view, while FIG. **2(b)** is a front view. It is noted that some of the constituent elements shown in FIG. **1** are omitted in FIG. **2** for the sake of ease of viewing. In an example, although the affixed part **115** may be transparent and thus the signal-acquiring section **110** may be visible from the back surface side thereof, the illustration of the signal-acquiring section **110** is omitted in FIG. **2**. The lower side in the diagram shown in FIG. **2(b)**, which corresponds to the front surface, is to be affixed and worn so as to come into contact with the forehead of a subject.

As shown in FIG. **2(a)** and FIG. **2(b)**, the substrate **500** and the rechargeable battery **320** are disposed so as to be stacked on the back surface side (upper side in the figure) of the affixed part **115** in the biosignal measurement apparatus **10** used as an electroencephalograph. The rechargeable battery **320** is connected to the substrate **500** via a cable **700**.

In the biosignal measurement apparatus **10** according to the present example, the affixed part **115**, which is an adhesive sheet freely expanded, contracted and bent as described above, has a shape and size approximately falling within the forehead of a human, in the plan view shown in FIG. **2(a)**. It is noted that the affixed part **115** is configured with an affixed part main body **115a** and a connecting part **115b** which form a series of sheets. The affixed part main body **115a** including the signal-acquiring section **110** has a substantially rectangular shape falling within an approximate size of a rectangle having a depth ( $D$  in the diagram) of 5 cm and a width ( $W$  in the diagram) of 15 cm. In view of the fact that the biosignal measurement apparatus **10** imparting less uncomfortable feeling during wearing is also suitable as an electroencephalograph for an infant, the affixed part main body **115a** is designed to have a size falling within the forehead of an infant. It is noted that each of the electrodes of the signal-acquiring section **110** is small enough so that the plurality of electrodes are enabled to be disposed with certain intervals on the affixed part **115** having even such a size. The connecting part **115b** includes the wiring (not shown in FIG. **2**) extending from the signal-acquiring section **110**. The wiring extends to the tip of the connecting part **115b** so as to be exposed. When the biosignal measurement apparatus **10** according to the present example is used, the connecting part **115b** having flexibility is bent so as to fold back the affixed part **115** having a sheet shape as described above, thereby falling within the size of the above-described rectangle in plan view.

As shown in FIG. **2(b)**, the substrate **500** is overlaid so as to face the back surface of the affixed part **115**. In the present

example, the substrate **500** is overlaid on the affixed part **115** via a cushion **600** made of an adhesive gel material. For example, a flexible substrate serves as the substrate **500**. Therefore, the substrate **500** along with the above-described cushion **600** provides a certain degree of followability to the shape of the forehead and the motion of the skin or the muscle of the subject wearing the biosignal measurement apparatus **10**, resulting in suppressing an uncomfortable feeling during wearing. A circuit (hereinafter also referred to as a signal processing circuit) for processing the biosignal acquired by the signal-acquiring section **110** is mounted on the flexible substrate. The tip of the connecting part **115b** is connected to the substrate **500** so that the biosignal acquired by the signal-acquiring section **110** is input to the signal processing circuit through the wiring. The substrate **500** will be detailed below.

The rechargeable battery **320**, which is a battery having a flexible sheet shape with a thickness of approx. 1 mm, and which is in a state of being connected to the substrate **500**, is overlaid so as to face the substrate **500** as shown in FIG. **2(b)**. A battery having a capacity according to use application is used. In an example, in the case where the biosignal measurement apparatus **10** is used to monitor a subject during sleep, a battery may be used, having a capacity allowing continuous use for 10 hours or longer, for example, a battery having the capacity of 200 mAh or more if the driving current of the biosignal measurement apparatus **10** is 20 mA.

In the biosignal measurement apparatus **10** according to the present example, the affixed part **115**, the cushion **600**, the substrate **500**, and the rechargeable battery **320** are stacked as described above. In plan view of the biosignal measurement apparatus **10** under such a state, the cushion **600**, the substrate **500**, and the rechargeable battery all fall within the size of the rectangular shape of the affixed part **115** described above. It is noted that a cable also falling within the size is used as the cable **700** for connecting the substrate **500** and the rechargeable battery **320**. The thickness ( $H$  in the figure) and weight of the entire biosignal measurement apparatus **10** are also suppressed to the utmost. The suppression of the size and weight as described above enables to impart less wearing feeling and less uncomfortable feeling to the subject wearing the biosignal measurement apparatus **10** on the forehead. In the case where the biosignal measurement apparatus **10** according to the embodiment described above has the configuration of the present example and has the substrate **500** and the rechargeable battery **320** falling within the outer shape of the affixed part **115**, the thickness and weight are reduced to the extents not exceeding 7 mm and 25 g, as an example. It is noted that in view of weight reduction, the affixed part **115** including the signal-acquiring section **110** is preferably formed as thin as possible, alternatively, in order to provide strength enough for practical handling, the affixed part **115** may be formed to have an appropriate thickness. In an example, in the case of the affixed part **115** having the size of the present example, the thickness of approx. 1 mm can provide practical strength.

FIG. **3** shows an example in which a subject wears the biosignal measurement apparatus **10** according to the present example. In FIG. **3**, the biosignal measurement apparatus **10** further covered with a cover not shown in FIG. **2** over the rechargeable battery **320** is affixed so that the front surface of the affixed part main body **115a** comes into contact with the forehead of the subject. As described above, the biosignal measurement apparatus **10** according to the present example is affixed on the forehead, like a commercially



## 11

available cooling gel sheet. The biosignal measurement apparatus **10** includes no cable and the like extending from the biosignal measurement apparatus **10** to the outside to transmit a signal or supply power, and thus the subject can freely move within a range in which measurement data is wirelessly transmitted to a destination. A mobile information terminal and storage unit, such as a notebook-type personal computer, tablet, and smartphone are used as a transmission destination of the measurement data, thereby enabling to further reduce the restriction in the motion range of the subject.

Electroencephalographs for research use or consumer use are conventionally used, having a simpler configuration compared to electroencephalographs for medical use. In each of these electroencephalographs, the electrodes thereof are fixed to the head of a subject with a fixing tool using elastic resin, rubber or the like. Such a fixing tool has upper and lower restriction in sizes applicable to the head. On the other hand, in the biosignal measurement apparatus **10** according to the present example, the electrodes are enabled to be fixed to the head of a subject without such a fixing tool, and thus the biosignal measurement apparatus **10** is available to, for example, an infant with a small circumference of the head. In the biosignal measurement apparatus **10** according to the present example, the head is not squeezed by a force unlike the case of an elastic fixing tool, and thus the biosignal measurement apparatus **10** is more likely to be used even with, for example, a subject who has injured his/her head, as compared with a conventional electroencephalograph.

## [2-2. Affixed Part and Signal-Acquiring Section]

FIG. **4** is a diagram illustrating a configuration example of the affixed part **115** including the signal-acquiring section **110**, and the substrate **500**, of the biosignal measurement apparatus **10** according to the present example shown in FIG. **2**. FIG. **4** shows that the affixed part **115** and the substrate **500** are in an unfolded state and are connected via a connector **350**.

In FIG. **4**, the eight hatched circles (**110a** to **110h**) provided in the affixed part main body **115a** correspond to the individual electrodes of the signal-acquiring section **110**. In the example shown in FIG. **4**, the affixed part **115** has two rows which parallelly extend in the longitudinal direction of the affixed part **115**, and each which includes four signal-acquiring sections **110** in line. Each of the hatched lines extending from each signal-acquiring section **110** to the right end of the connecting part **115b** corresponds to the wiring serving as a path of a biosignal. It is noted that the signal-acquiring section **110** is not limited to the present example in the shape, the number, the number of rows, and the positional relation among the signal-acquiring sections **110**. The wiring pattern is not limited to the example shown in FIG. **4**.

As described above, these signal-acquiring sections **110** include a reference electrode for acquiring a reference potential, and a measurement electrode for measuring a potential difference from the reference potential at each position. In an example, a signal-acquiring section **110a** may be a reference electrode, while a signal-acquiring section **110b** may be a measurement electrode for measuring a potential difference from the reference potential acquired by the signal-acquiring section **110a**. That is, the signal-acquiring section **110a** is the reference electrode to the signal-acquiring section **110b** which is a measurement electrode. Similarly, a signal-acquiring section **110c** may be the reference electrode to a signal-acquiring section **110d** which is a measurement electrode; a signal-acquiring section **110e** may

## 12

be the reference electrode to a signal-acquiring section **110f** which is a measurement electrode; and a signal-acquiring section **110g** may be the reference electrode to a signal-acquiring section **110h** which is a measurement electrode. In this case, the biosignal measurement apparatus **10** is capable of measuring biosignals with four channels. Alternatively, the signal-acquiring section **110a** may be the reference electrode to the signal-acquiring sections **110b** to **110h** which are measurement electrodes. In this case, the biosignal measurement apparatus **10** is capable of measuring biosignals with 7 channels. It is noted that the number of the signal-acquiring sections **110** is not limited to that in the above-described example, and alternatively, biosignals may be measured with more channels by use of more signal-acquiring sections **110**.

The plurality of signal-acquiring sections **110** may include an electrode attachable to and detachable from the affixed part **115**, and the electrode may be used as a reference electrode for measuring a reference potential at a position other than the forehead, such as the earlobe. As in the example shown in FIG. **5**, the signal-acquiring section **110a** may be a reference electrode detachable from the affixed part main body **115a**. FIG. **5** is a diagram illustrating another example of the configuration of the affixed part **115** including the signal-acquiring section **110**, and the substrate **500**, of the biosignal measurement apparatus **10** according to the present example shown in FIG. **2**. FIG. **5** shows the state where the signal-acquiring section **110a** having been affixed on the position indicated by the broken line is peeled off and detached from the affixed part main body **115a**. It is noted that the signal-acquiring section **110** detached from the affixed part main body **115a** is still in connection with the wiring serving as a path of a signal. The signal-acquiring section **110** once having been peeled off from the affixed part main body **115a** as described above is enabled to be affixed again to the affixed part **115** due to the adhesiveness of the affixed part **115**.

Although the connecting part **115b** has flexibility as described above, the degree of flexibility may be changed depending on the location. In an example, the stress caused by energizing in the routing in the biosignal measurement apparatus **10** and/or by deformation of the connecting part **115b** concentrates at the tip portion of the connecting part **115b** to be engaged with the connector **350** for connection to the substrate **500**. In the case of the connecting part **115b** made of flexible material like the affixed part main body **115a**, such stress likely breaks the tip portion. In order to prevent such premature breakage, the connecting part **115b** as an example may be configured so as to increase in hardness from the portion close to the signal-acquiring section **110** (the affixed part main body **115a**) toward the portion close to the tip thereof. In an example, in FIG. **4**, an area A, that is, the affixed part main body **115a** and a part closer to the affixed part main body **115a** of the connecting part **115b**, are both made of a flexible silicone material having the above-described expandability and contractibility. An area B next to the area A may be made of a plastic resin which has flexibility of such an extent allowing easy bending and which has lower expandability and contractibility compared to that of the area A. An area C next to the area B including the tip of the connecting part **115b** may be made of a plastic resin which has flexibility and lower expandability and contractibility like the area B, and which is harder than the plastic resin of the area B. In such a configuration, the stress as described above is dispersed also to the portions of the boundaries of the materials in the connecting part **115b**, not concentrating at the tip portion of



the connecting part **115b**. This delays the breakage of the connecting part **115b** due to the stress, thereby enabling to prolong the service life of the affixed part **115**.

[2-3. Substrate]

The signal processing circuit is mounted on the substrate **500** as described above. The signal processing circuit herein includes the amplifying section **120** and the A/D converting section **130** of the input unit **100**, the control unit **200**, the charging circuit **310** of the power source unit **300**, and the output unit **400**. Each of these constituent elements is classified as an analog circuit, a digital circuit or a power source circuit. The analog circuits include the amplifying section **120** and the A/D converting section **130** for processing the analog signal acquired by measuring a potential on the body surface of a living body to convert it into a digital signal. The digital circuits include the CPU **210**, the base band DSP **220**, the contact state-detecting section **230** and the clock-generating section **240** of the control unit **200**, and the output unit **400** for wirelessly transmitting the processed digital signal, which are related to processing of a digital signal. The power source circuits include the power source-managing section **250** and the electric power-stabilizing section **260** of the control unit **200**, and the charging circuit **310** and the rechargeable battery **320** of the power source unit **300**, which supply power to the analog circuits and the digital circuits. These analog circuits, the digital circuits and the power source circuits are respectively mounted in a first region, a second region and a third region which are obtained by dividing the mounting surface of the substrate **500** into three regions. In an example, in FIG. 4, the area indicated by a is the first region, the area indicated by c is the second region, and the area indicated by b is the third region. The region for the analog circuits is separated from the region for the digital circuits in such a manner, thereby suppressing noise generated on one side from coming into the other side. The voltages of the driving powers are different between the analog circuits and the digital circuits, and thus the output systems from the rechargeable battery **320** are different between the analog circuits and the digital circuits. On the other hand, a GND line is common between the analog circuits and the digital circuits. Accordingly, the region in which the analog circuits are mounted and the region in which the digital circuits are mounted are separated as much as possible in the substrate **500**, thereby suppressing the influence by noise.

It is noted that although the shapes and sizes of the respective regions obtained by dividing the substrate **500** are substantially the same in the example shown in FIG. 4, the method of dividing the substrate **500** in the present invention is not limited to that in the present example. The substrate **500** may not be of one physically-continuing sheet of a flexible substrate. In an example, each or some of the first region to the third region may be mounted on a separate flexible substrate, and these flexible substrates may be connected by wiring to transmit a signal and supply power.

The rechargeable battery **320** included in the power source circuits may not be mounted on the substrate **500**. In an example, the rechargeable battery **320** may be mounted on the substrate **500** via a holder provided on the substrate **500**, or may be connected to a flexible substrate via a cable as shown in FIG. 2.

Although the substrate **500** is a flexible substrate in the case described above, the substrate **500** is not limited to a flexible substrate. That is, the substrate **500** may be a rigid substrate. Even in the case where the substrate **500** is a rigid substrate, the substrate **500** is formed as small as possible in size occupied in the biosignal measurement apparatus **10**,

whereby less uncomfortable feeling is imparted by the substrate **500** to the subject via the cushion **600** and the affixed part **115**.

[2-4. Precision]

The biosignal measurement apparatus **10** according to the present example is rather small and is easily used as compared with a conventional brain wave measuring apparatus for medical use. However, unless the precision in measurement of a biosignal by the apparatus is sufficient, the apparatus is not suitable for use as a medical instrument.

FIG. 6A and FIG. 6B are the electroencephalograms obtained by concurrently measuring brain waves of one subject by use of both of the biosignal measurement apparatus **10** according to the present example and a brain wave measuring apparatus for medical use (Neurofax (registered trademark) EEG-1200 manufactured by Nihon Kohden Corporation, hereinafter referred to as Neurofax) affixed on the forehead. It is noted that the reference potential is acquired at the earlobe. FIG. 6A shows the electroencephalogram of the brain waves measured in the state where the eyes of the subject are open, while FIG. 6B shows the electroencephalogram of the brain waves measured in the state where the eyes of the subject are open. Each of the solid lines in the curves of these electroencephalograms shows the brain waves acquired by the biosignal measurement apparatus **10** according to the present example, while each of the broken lines shows the brain waves acquired by Neurofax. These electroencephalograms reveal that the brain waves acquired by the both apparatuses are consistent with each other at a high level. The results of the frequency analysis of the acquired brain waves also reveal high consistency therebetween, and further reveal that the brain waves acquired by the both apparatuses have high correlation, with a correlation coefficient of 0.99 or more. As described above, the biosignal measurement apparatus **10** according to the present example is capable of measuring a minute potential variation, for example, brain waves with precision comparable to that of a brain wave measuring apparatus for medical use.

[2-5. Application Example]

The biosignal measurement apparatus **10** according to the present example for use as an electroencephalograph is capable of measuring brain waves with ease and less burden on a wearing subject as compared with a conventional electroencephalograph for medical use or other use. A subject wearing the biosignal measurement apparatus **10** can move and work in some degree. That is, the biosignal measurement apparatus **10** allows continuous measuring of brain waves under a state close to everyday life by using it as a so-called wearable device.

The biosignal measurement apparatus **10** for use as an electroencephalograph as described above is used for, for example, sleep state management at home of a patient of sleep apnea syndrome, quantitative assessment based on brain activity data of ability of the elderly such as in driving or machine work, monitoring and diagnosis by quantitative assessment based on brain activity such as of dementia with abnormal brain activity, Parkinson's disease, epilepsy, psychiatric disorder and the like, monitoring of depth of anesthesia during surgery, research for brain development science, and the like.

In the field of drug discovery, the biosignal measurement apparatus **10** is available for collection of data on the quantitative variation in brain activity caused by administration of medicine for a nervous system. In the field of medical care, the biosignal measurement apparatus **10** is available for collection of data serving as an index for



selecting the optimum medicine for a patient from a plurality of medicines having the same purpose.

In the field of nursing care, even in the case of a care receiver having difficulty in communication, the biosignal measurement apparatus **10** is available for monitoring of such a care receiver to detect temperature and discomfort such as pain on the basis of brain waves.

Furthermore, in view of a product to be put to practical use, the biosignal measurement apparatus **10** is expected to be provided at a smaller cost to a subject as compared with a conventional electroencephalograph. This facilitates introduction of the biosignal measurement apparatus **10** to individuals, thereby encouraging the realization of healthcare monitoring aimed at individualized medical care. In some fields other than medical care, the biosignal measurement apparatus **10** is expected to be used by an individual as a user interface of means for controlling a device on the basis of brain waves, means for switching between automatic operation and manual operation for a device on the basis of brain waves, and the like.

### [3. Other Application Examples]

In the description of the above examples, the biosignal measurement apparatus **10** is used as an electroencephalograph. Alternatively, as described above, the biosignal measurement apparatus **10** is applicable to an apparatus for measuring a biosignal on the basis of each type of a potential, such as an electrocardiograph, an eye movement electrometer, an electromyograph or the like. The biosignal measurement apparatus **10** is provided also as the above measurement apparatus, imparting less wearing feeling with sufficient precision, as compared with conventional apparatus.

It is noted that the biosignal measurement apparatus **10** provided as such an apparatus for measuring a biosignal other than brain waves has the same basic configuration as that in the above-described embodiment, in which appropriate change is made for adjustment with regard to the number and arrangement of the electrodes serving as the signal-acquiring section **110**, the shape and size of the affixed part **115** covering a measurement portion, a processing algorithm for visualizing the acquired biosignals, and the like.

Such a measurement apparatus is available as, for example, an electromyograph at home for a uterus of a pregnant woman for early detection of the timing of a delivery. Such a measurement apparatus is also available as monitoring means in the case where a fetus has abnormality in health condition or as a heart rate meter for a fetus used as a communication tool with the fetus.

The biosignal measurement apparatus **10** is also available for collection of data on body control in sports, rehabilitation, or the like. In such use application, the biosignal measurement apparatus **10** according to the present invention has advantages in imparting less wearing feeling and providing fewer disturbances in exercise, and in having redundancy allowing continuous measurement even under disconnection of some electrodes caused by exercising.

In the case of such use application, the shape and size of the affixed part **115** are not limited to those in the above-described examples, and are appropriately determined in consideration of, for example, the number and arrangement of the signal-acquiring sections **110** according to each use application, and in consideration of the stability of the affixed biosignal measurement apparatus **10** and the wearing feeling imparted to a subject while wearing.

Because wearing feeling is less, the biosignal measurement apparatus **10** is available for simultaneous measure-

ment of brain waves and other biosignals with relatively light burden on a subject by using together with the above-described electroencephalograph.

Although the present invention has been described using embodiments and examples of a biosignal measurement apparatus for a human body, the present invention is applicable to measurement of a potential variation of a living body other than a human body or an object other than a living body. In an example, the variation in potential difference on the surface of a plant is monitored, thereby enabling to control growth of an agricultural crop; and in another example, the potential difference on the surface of a concrete portion of a building is mapped, thereby enabling to detect an internal state, such as regarding whether or not internal corrosion occurs. It is noted that in the case of such use application to an object other than a human body, the shape and size of the affixed part **115** are not limited to those in the above examples, and are appropriately determined, for example, in consideration of the number and arrangement of the signal-acquiring sections **110** according to each use application, and in consideration of the stability of the affixed biosignal measurement apparatus **10**.

### [4. Modifications]

Although the biosignal measurement apparatus according to the present invention has been described using the embodiments and examples, the present invention is not limited to the above-described embodiments or examples. Modifications made in the biosignal measurement apparatus according to the present invention are described below.

In an example, the above-described biosignal measurement apparatus **10** may not include the cushion **600** provided between the substrate **500** and the affixed part **115**. In an example, the substrate **500** may be directly fixed to the affixed part **115**, or may be fixed to the cover shown in FIG. **3**. The substrate **500** and the affixed part **115** may not be arranged so as to be stacked. In an example, the substrate **500** and the affixed part **115** may be used in an unfolded state as shown in FIG. **4** without being bent at the connecting part.

The biosignal measurement apparatus **10** may further include a storage unit for storing biosignal data. The storage unit is used as, for example, a temporary storage location of data in case where wireless communication with the outside is not available. The data may be output to the outside via the output unit **400** in a state where wireless communication is available. The biosignal measurement apparatus **10** may be configured so that data is output also through an attachable and detachable communication cable. In an example, data may be output through a cable connected to the USB port included in the charging circuit **310**.

A power source by environmental power generation using light, vibration or the like may be used additionally, depending on the place or motion of the subject wearing the biosignal measurement apparatus **10**, and the use application of the biosignal measurement apparatus. This enables to prolong the continuous use period of time. It is noted that the duration of the battery is adjustable by changing the number of channels, the sampling rate of the analog signal or the like within a range in which measurement data required for each use application is acquired.

The affixed part **115**, which is a sheet on which the signal-acquiring section **110** of electrodes and wiring are formed, is made of any material as long as it is freely expanded, contracted and bent and is adhesive as described above, and the material is not limited to silicone. In an example, the affixed part **115** may be a sheet like a court-



17

plaster, made of resin, rubber, fiber (cloth) or other material, or a sheet of a combination thereof having similar characteristics.

The material used for the expandable and contractible conductor of which the signal-acquiring section **110** and wiring are made is not limited to the above-described silver nanowire. Nanowire made of other metal such as gold or copper which are conductors, or carbon nanofiber may be used instead, or a mixture thereof may be used.

The embodiments and the modifications thereof have been described so far as examples for the purpose of explaining the technical contents of the present invention. Accordingly, the technical scope of the invention according to the present application is not limited to the description. The technical scope of the invention according to the present application includes every possible change, replacement, addition, and omission made by those skilled in the art within the range of the specification, drawings and claims, or within the equivalents thereto.

#### INDUSTRIAL APPLICABILITY

The present invention is applicable to a biosignal measurement apparatus such as an electroencephalograph, an electrocardiograph, an eye movement electrometer, and an electromyograph, and is also applicable to an apparatus for measuring a potential of an object other than a living body, such as of the surface of a building.

#### EXPLANATION OF REFERENCE NUMERALS

**10** BIOSIGNAL MEASUREMENT APPARATUS  
**100** INPUT UNIT  
**110, 110A TO 110H** SIGNAL-ACQUIRING SECTION  
**115** AFFIXED PART  
**115a** AFFIXED PART MAIN BODY  
**115b** CONNECTING PART  
**120** AMPLIFYING SECTION  
**130** A/D CONVERTING SECTION  
**200** CONTROL UNIT  
**210** CPU  
**220** BASE BAND DSP  
**230** CONTACT STATE-DETECTING SECTION  
**240** CLOCK-GENERATING SECTION  
**250** POWER SOURCE-MANAGING SECTION  
**260** ELECTRIC POWER-STABILIZING SECTION  
**300** POWER SOURCE UNIT  
**310** CHARGING CIRCUIT  
**320** RECHARGEABLE BATTERY  
**330** CONNECTION TERMINAL  
**350** CONNECTOR  
**400** OUTPUT UNIT  
**500** SUBSTRATE  
**600** CUSHION  
**700** CABLE

What is claimed is:

**1.** A biosignal measurement apparatus used by being affixed on a living body, the biosignal measurement apparatus comprising:

a sheet formed with a plurality of electrodes and a plurality of wirings connected to the plurality of electrodes respectively, the sheet being freely expanded, contracted and bent and being adhesive, wherein the sheet has a flexible connecting part;

a connector attached to a tip of the flexible connecting part and connected to the plurality of wirings disposed on the sheet; and

18

a substrate connected to the connector and equipped with a signal processing circuit wirelessly transmitting a biosignal acquired via the plurality of wirings disposed on the connector,

wherein the sheet is physically separated from the substrate, and the sheet is only connected to the substrate via the connector,

wherein the plurality of electrodes are exposed on a front surface of the sheet, and the sheet and the substrate are stacked so that a back surface of the sheet faces the substrate.

**2.** The biosignal measurement apparatus according to claim **1**, wherein

each of the sheet and the substrate under a state of the front surface of the sheet affixed on the living body has an outer shape in plan view of a size falling within a rectangle of 5 cm×15 cm.

**3.** The biosignal measurement apparatus according to claim **1**, wherein

the plurality of electrodes include a reference electrode and a plurality of measurement electrodes.

**4.** The biosignal measurement apparatus according to claim **3**, wherein

the reference electrode is attachable to and detachable from the sheet, and is affixed on the sheet.

**5.** The biosignal measurement apparatus according to claim **1**, wherein

the plurality of electrodes include electrodes arranged parallelly in at least two rows, and each of the rows includes a plurality of electrodes in line.

**6.** The biosignal measurement apparatus according to claim **1**, wherein

the plurality of wirings extend respectively and correspondingly from the electrodes to the connecting part, and

the connecting part is bent so that the sheet is folded back, and a tip of the connecting part is connected to the signal processing circuit.

**7.** The biosignal measurement apparatus according to claim **6**, wherein

the connecting part of the sheet increases in hardness from a portion close to the plurality of electrodes toward a portion close to the tip.

**8.** The biosignal measurement apparatus according to claim **1**, wherein

the signal processing circuit includes an analog circuit for processing an analog signal acquired via the plurality of electrodes to convert the analog signal into a digital signal, a digital circuit for processing the digital signal acquired by the analog circuit to transmit the digital signal wirelessly, and a power source circuit for supplying power to the analog circuit and the digital circuit, and

the analog circuit, the digital circuit and the power source circuit are respectively mounted in a first region, a second region and a third region obtained by dividing a mounting surface of the substrate into three regions.

**9.** The biosignal measurement apparatus according to claim **8**, wherein

the analog circuit has an A/D converting section for converting the analog signal into a digital signal having a bit number of 20 bits or more.

**10.** The biosignal measurement apparatus according to claim **8**, wherein

the analog circuit has a contact state-detecting circuit for detecting a contact state between the plurality of elec-



trodes and the living body by measuring a contact impedance between the plurality of electrodes and the living body.

11. The biosignal measurement apparatus according to claim 8, wherein the power source circuit includes: 5  
a rechargeable battery;  
a connection terminal provided on the substrate; and  
a charging circuit for charging the battery with power supplied through the connection terminal.

12. The biosignal measurement apparatus according to 10  
claim 1, further comprising a cushion between the sheet and the substrate.

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