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(54) ADJUSTABLE KNOTLESS LOOPS

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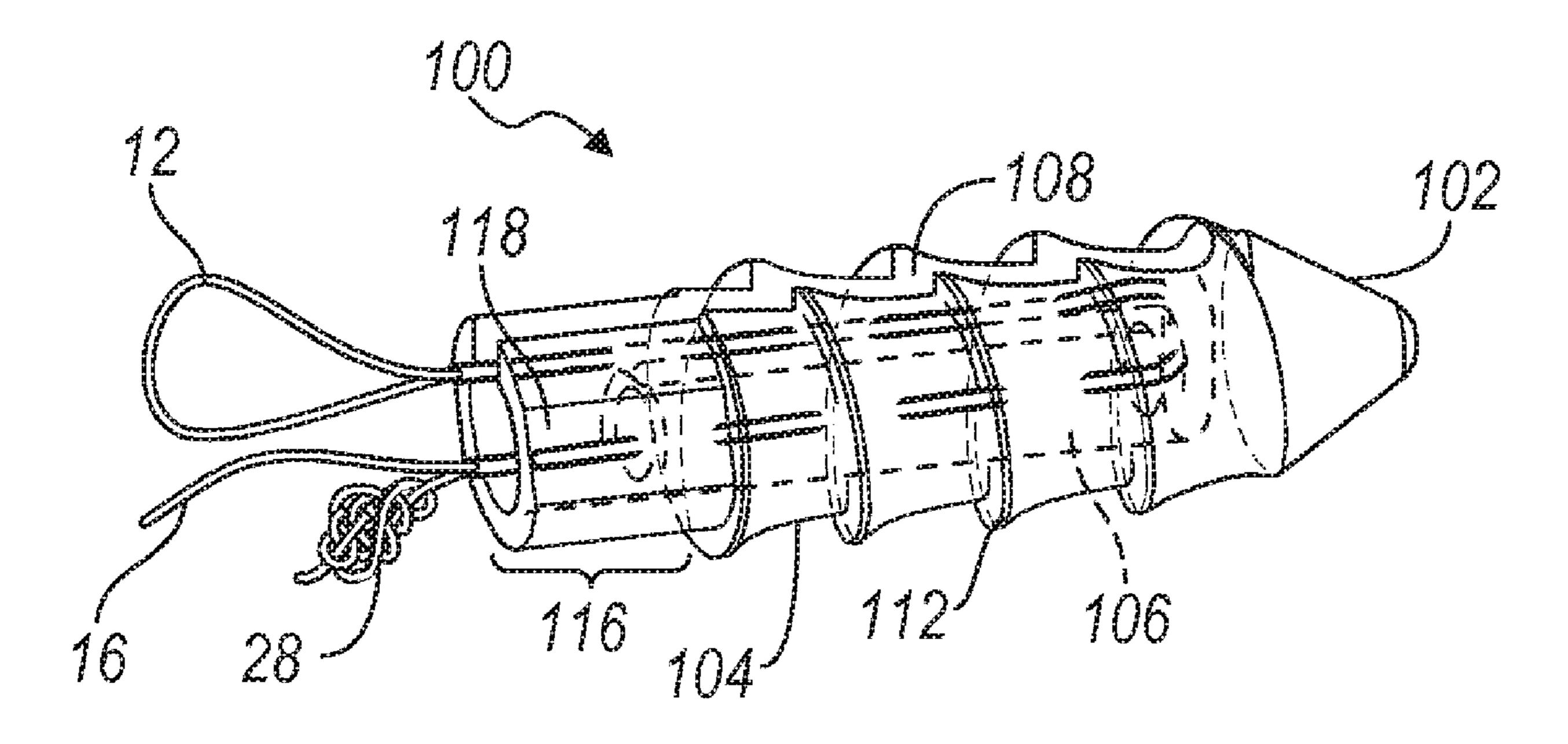
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(57) ABSTRACT

Methods of attaching a soft tissue to an adjacent bone at a defect site are provided. An adjustable loop region of a flexible construct contained in a bore defined by a fastener is passed through a tissue. The adjustable loop is passed through the tissue. The fastener is passed back through the adjustable loop to fold the adjustable loop upon itself. The fastener is attached to the bone. An adjusting arm on the flexible construct is engaged to reduce the size of the adjustable loop and secure the soft tissue to the bone.

14 Claims, 8 Drawing Sheets



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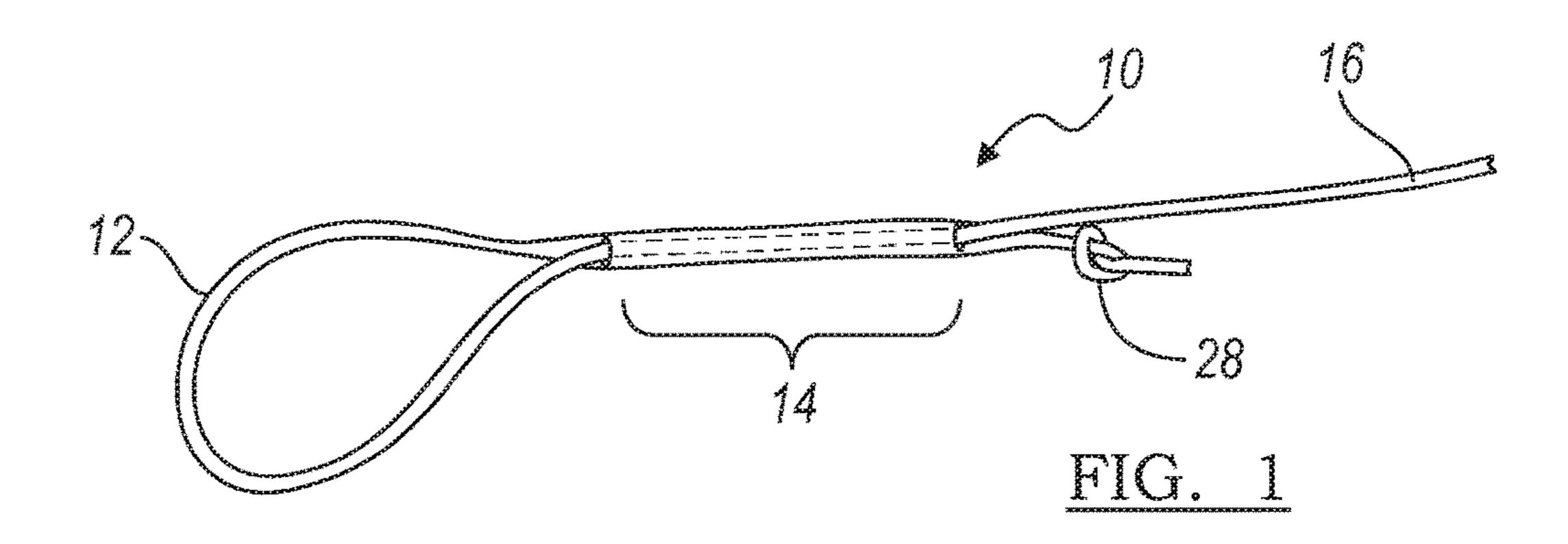
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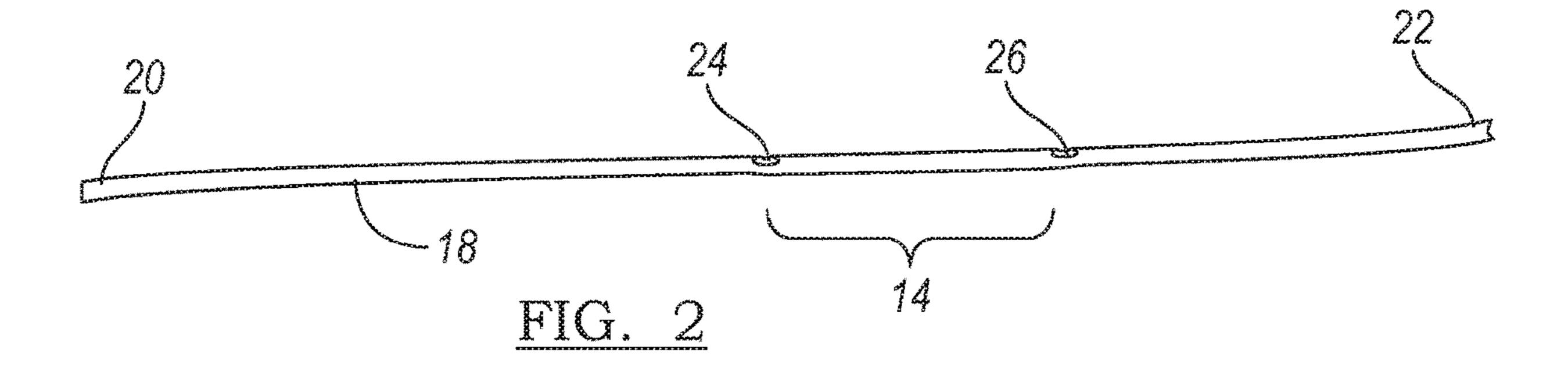
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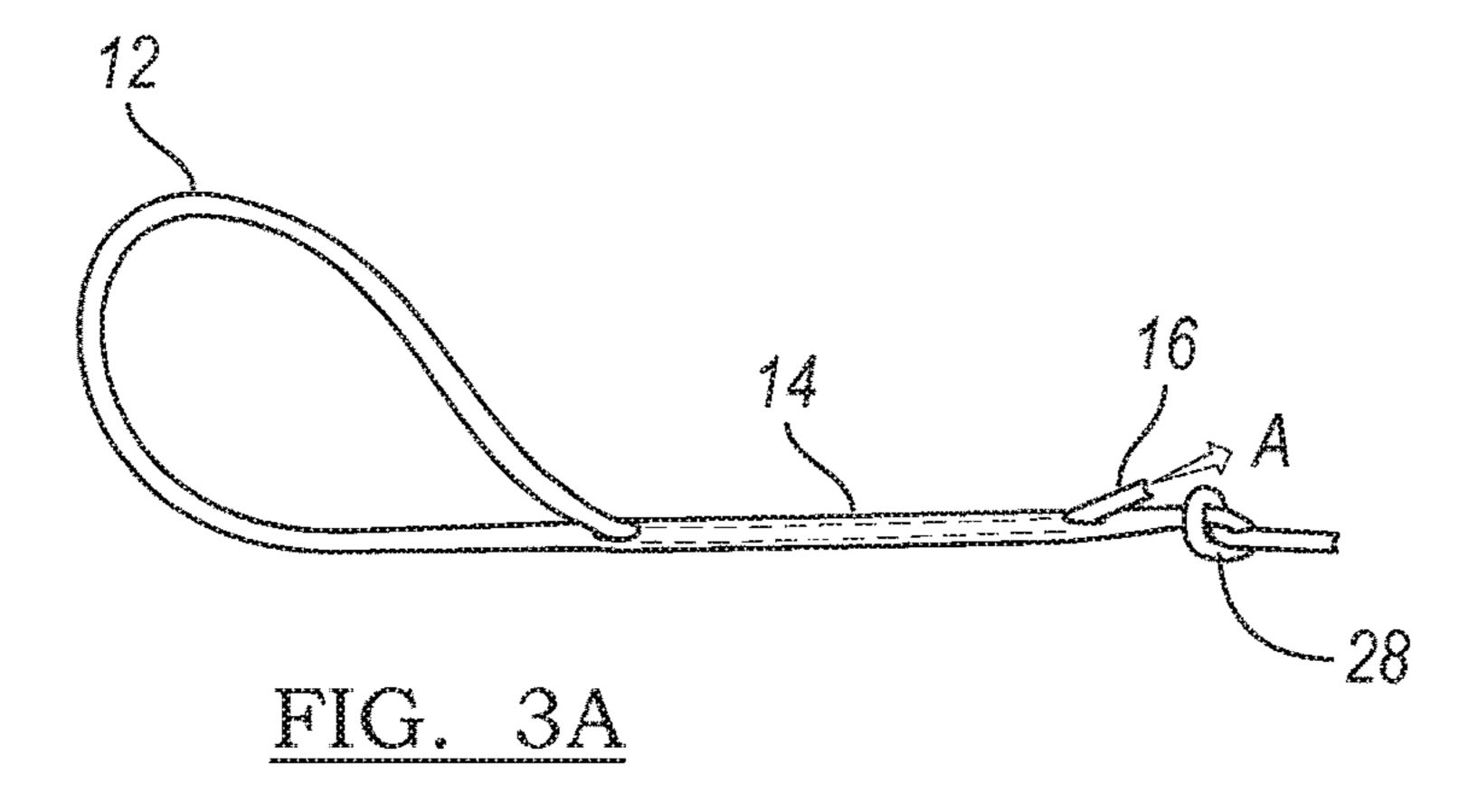
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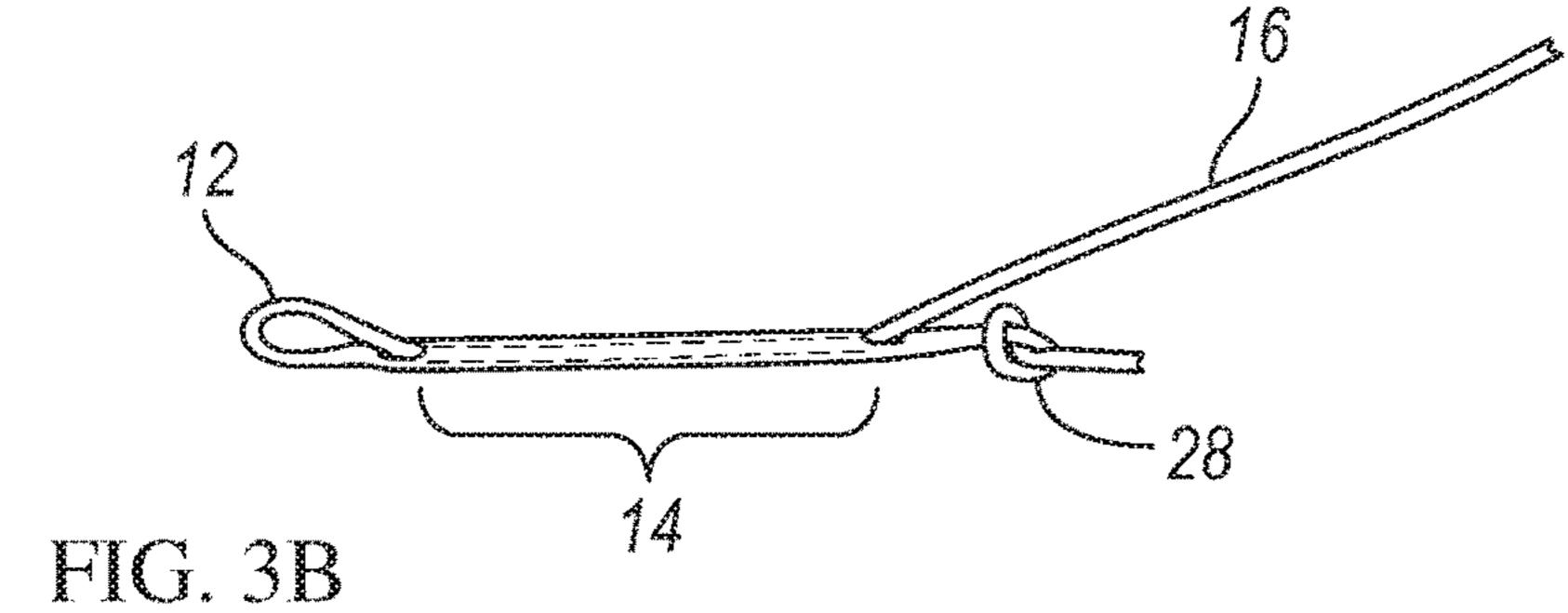
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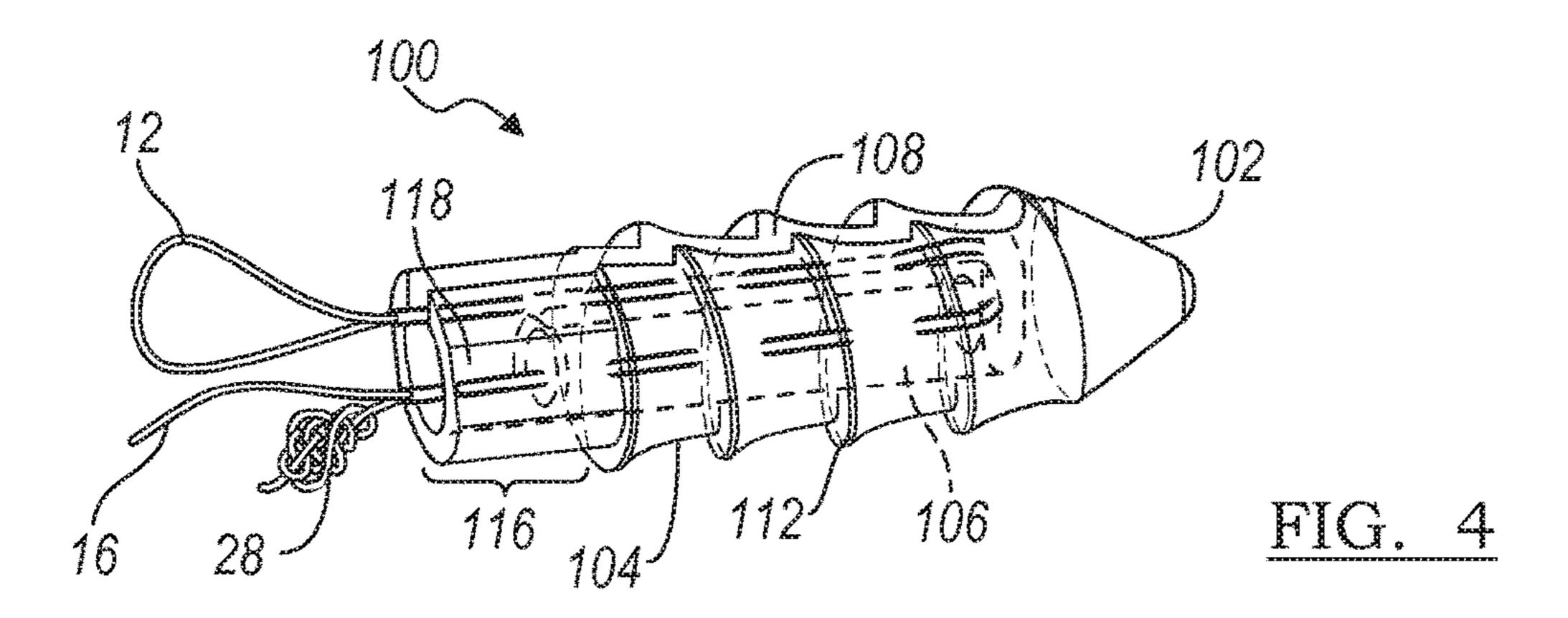
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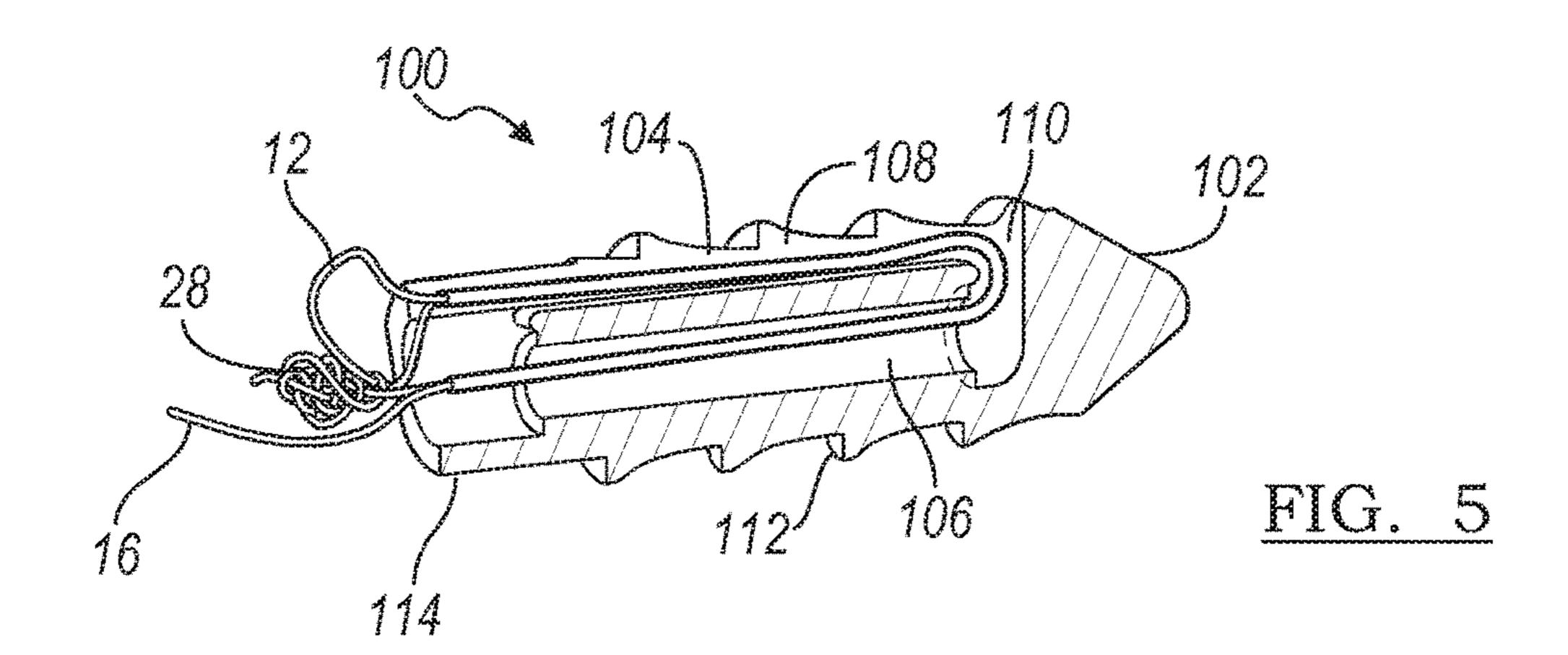












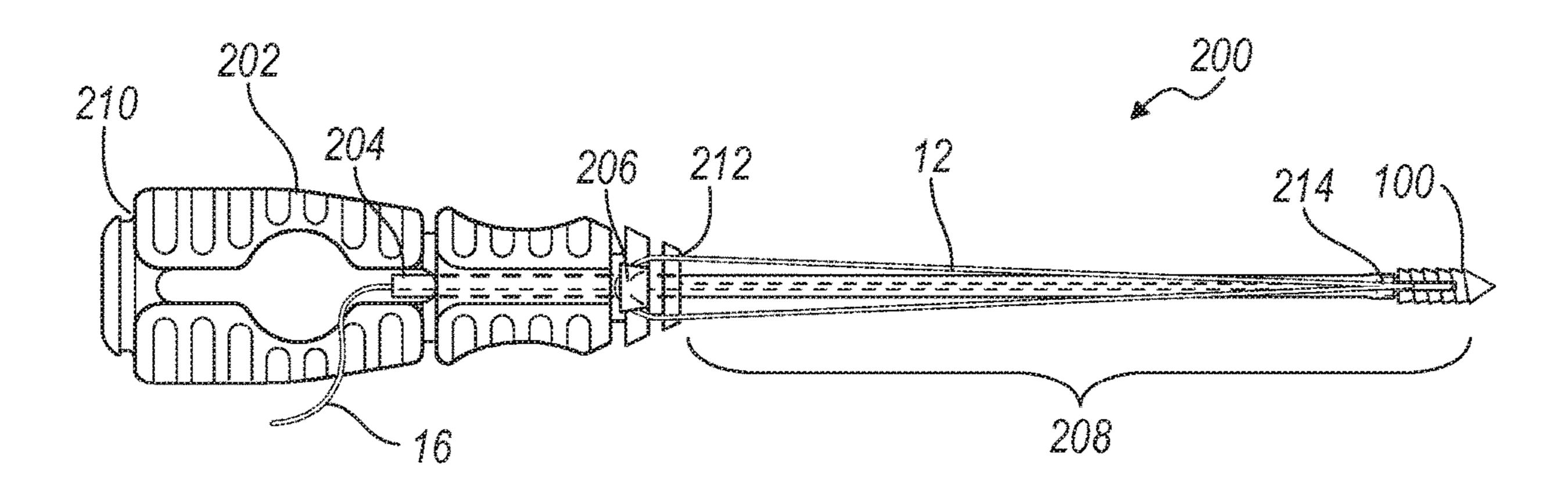


FIG. 6

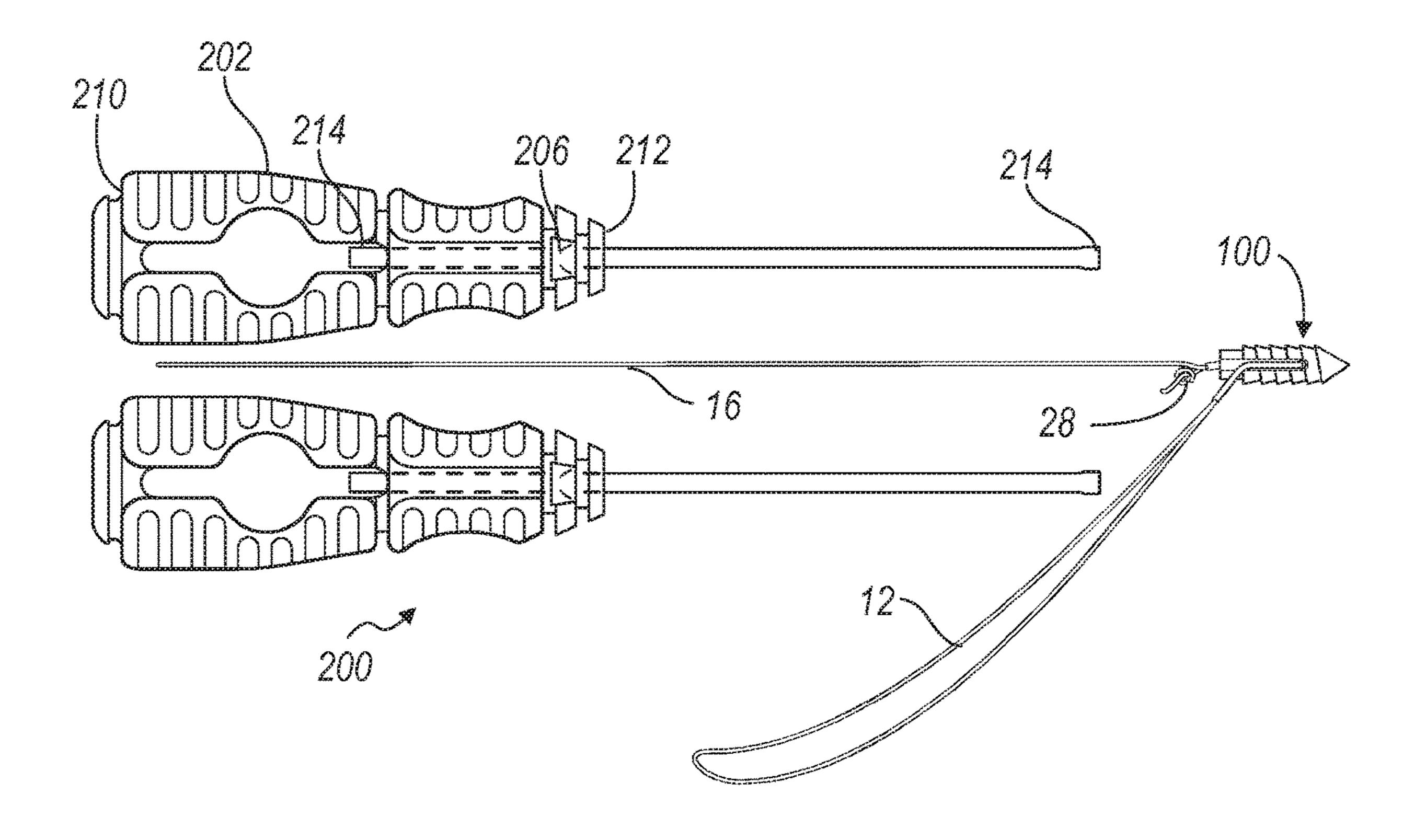
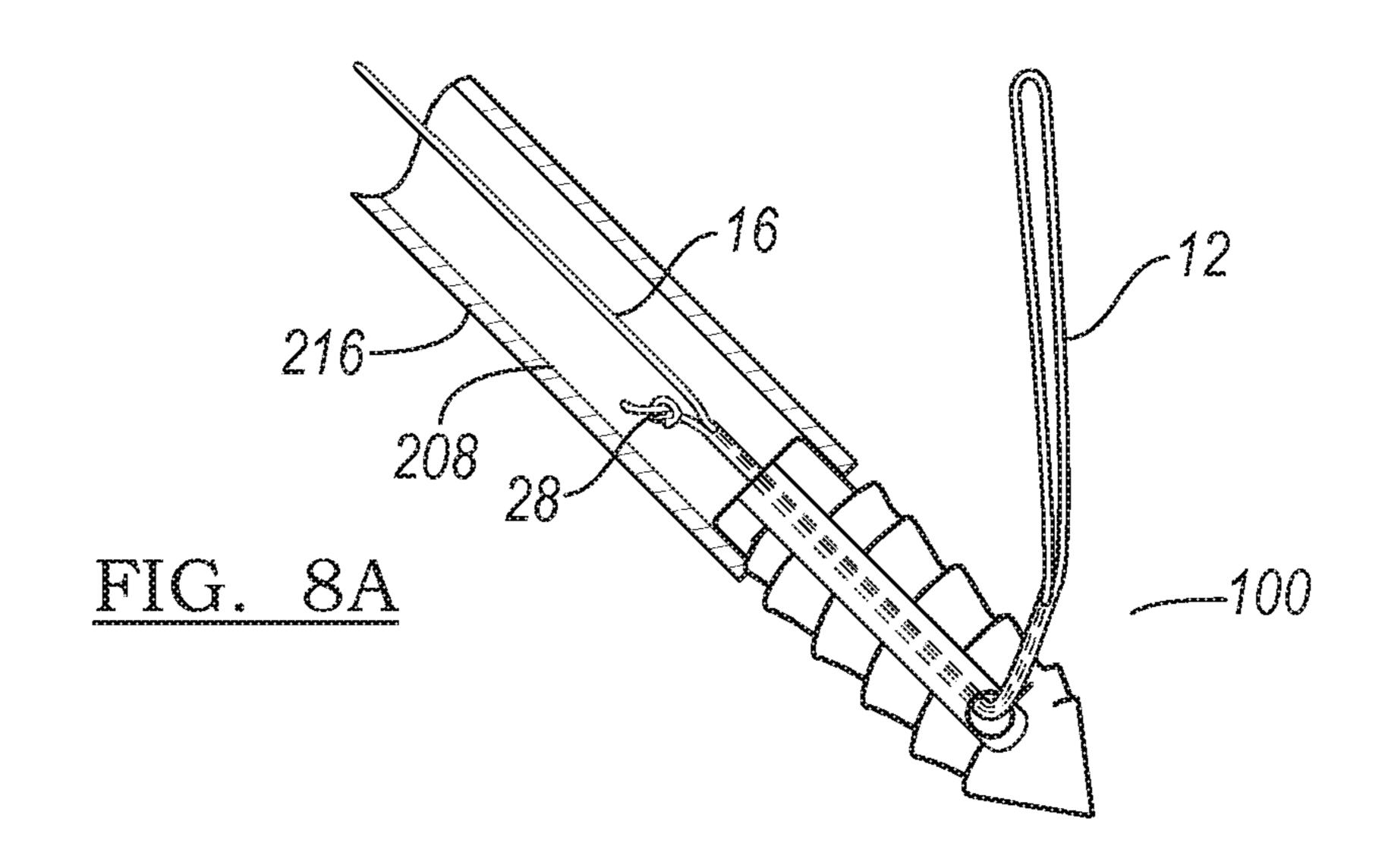
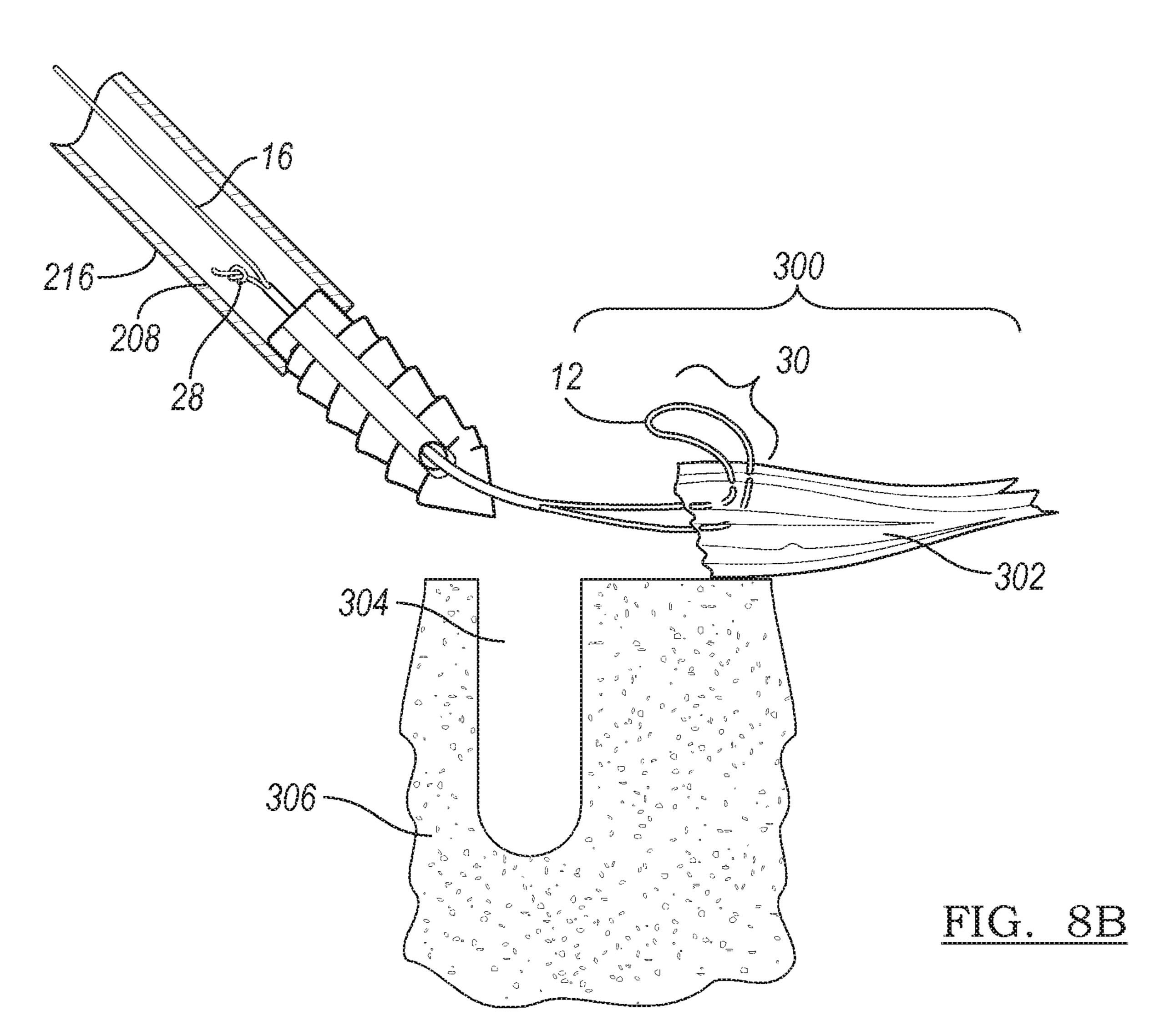


FIG. 7





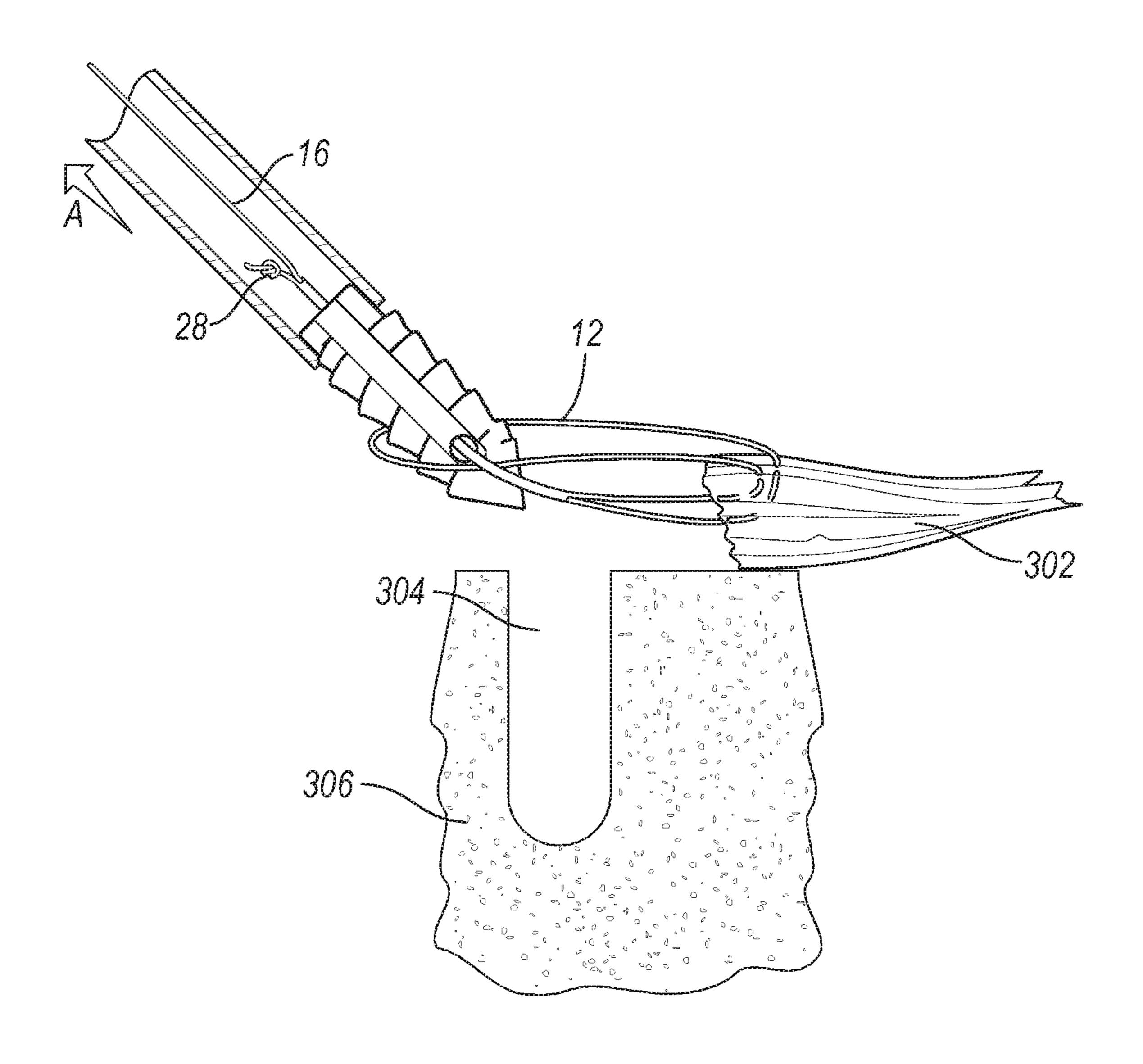
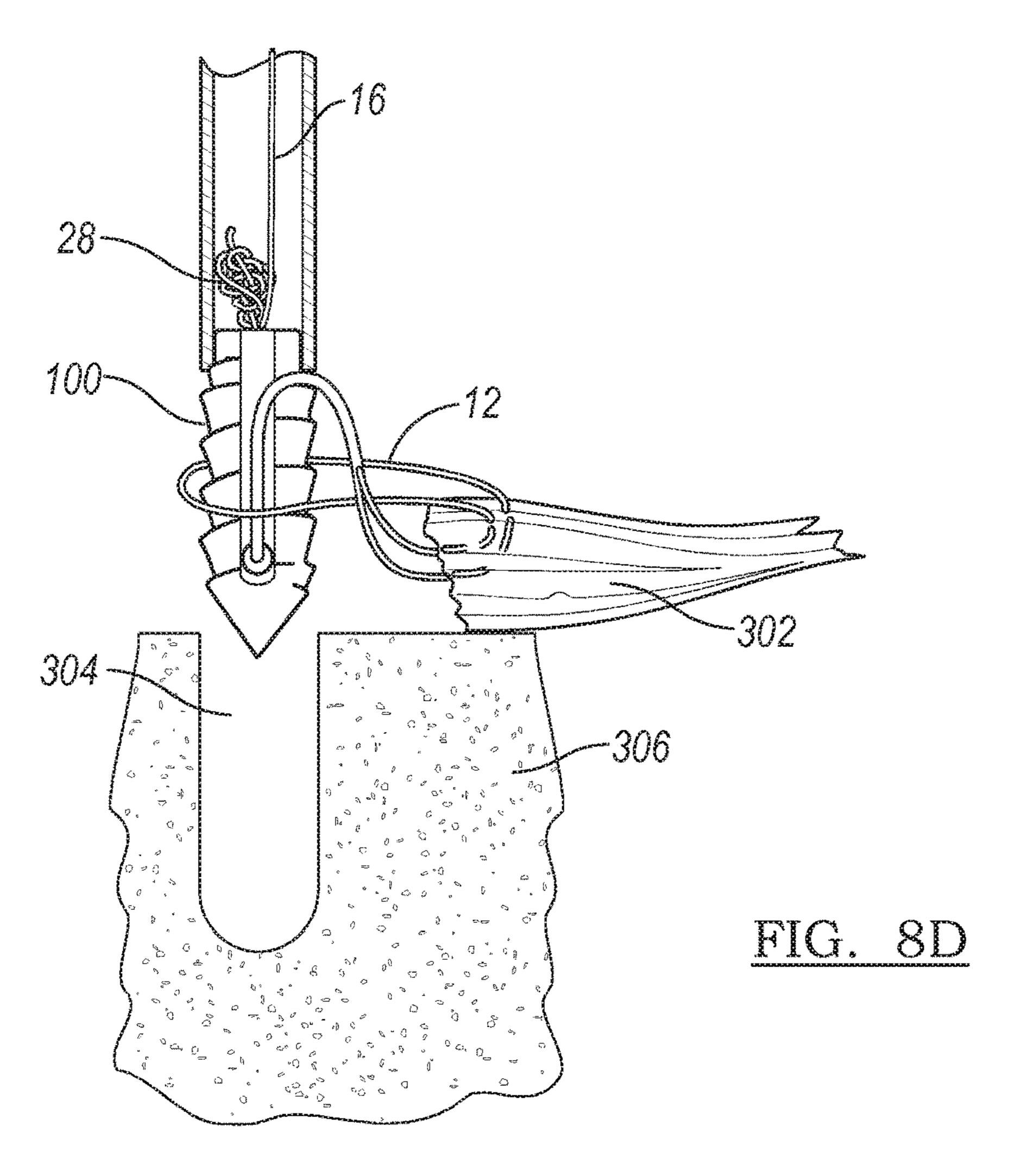
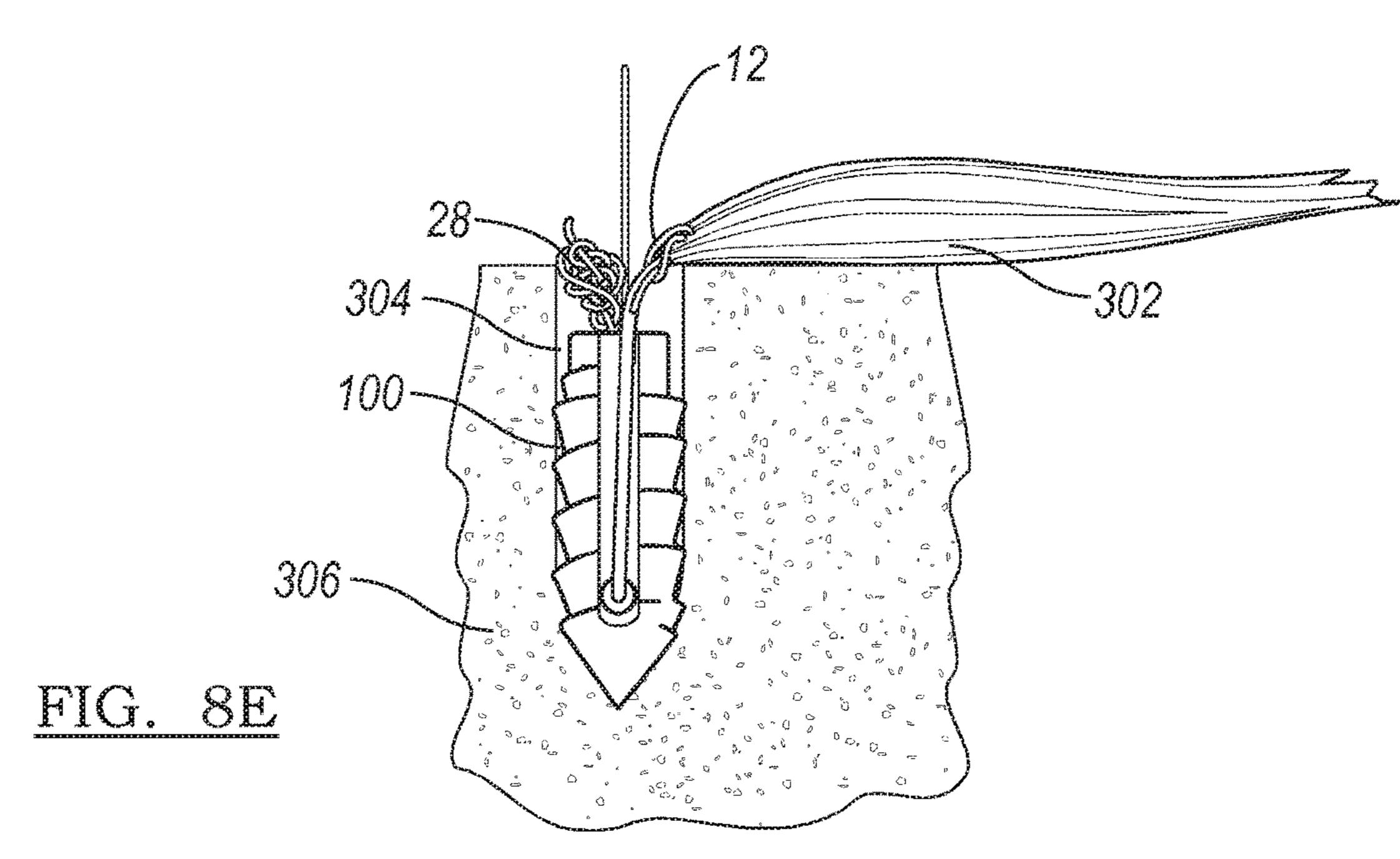
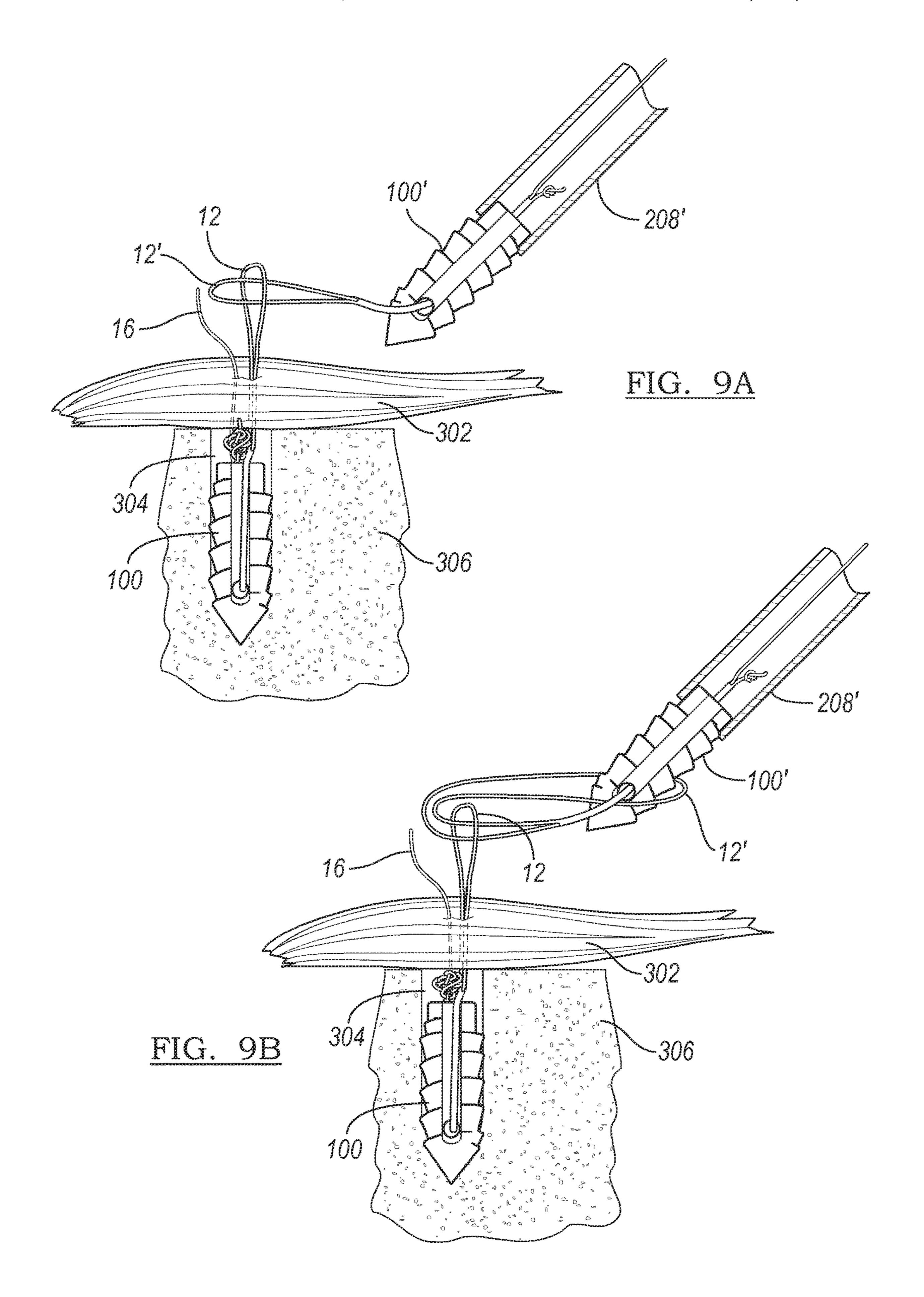
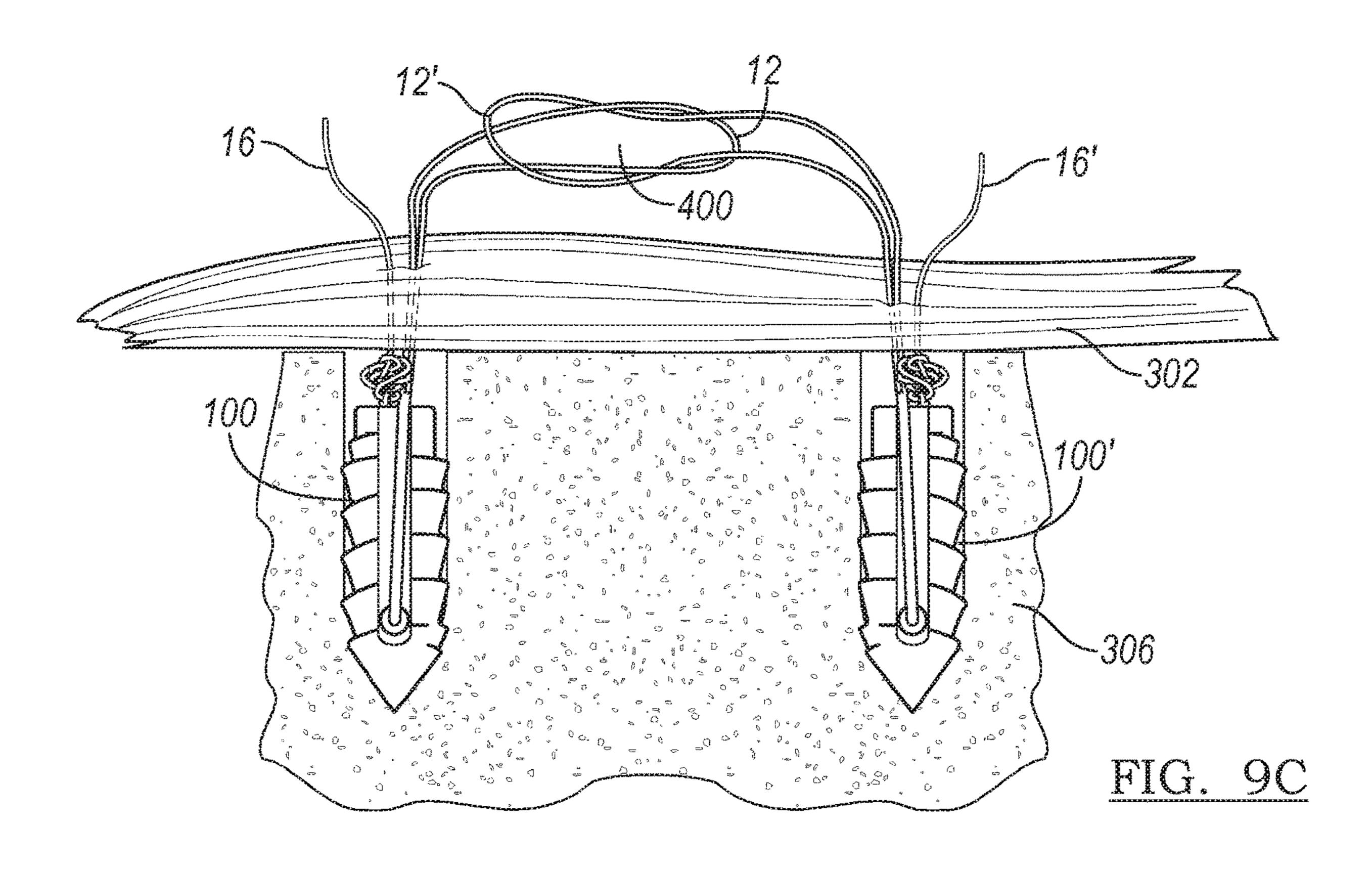


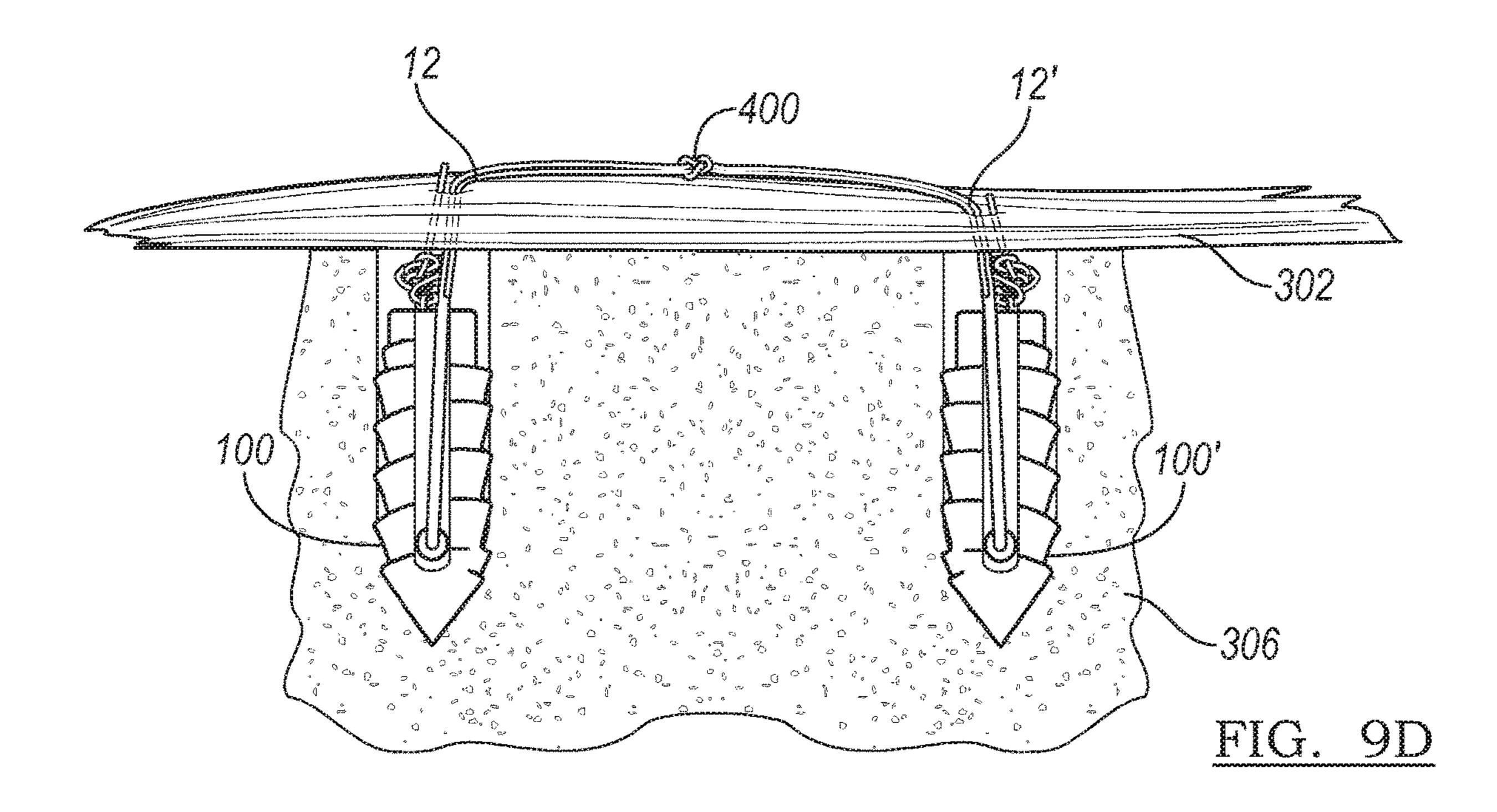
FIG. 8C











ADJUSTABLE KNOTLESS LOOPS

FIELD

The present disclosure relates to methods and apparatuses of for securing a flexible construct. In particular, the present disclosure relates to securing a flexible construct with an adjustable loop.

BACKGROUND

The statements in this section merely provide background information related to the present disclosure and may not constitute prior art.

Surgical procedures are often performed on a body, for 15 example, a human body or anatomy, to repair or replace various portions thereof. For example, the soft tissues of the body may need to be reattached to bones due to trauma, overuse, surgical intervention, or disease.

Soft tissues can be reattached to bone using fastening devices such as screws, staples, and various types of suture anchors. Soft tissues are often fixed to various positions on the bone. For example, to replace a natural tendon fixation point or to replace the tendon itself, fixing a graft to a selected bone area may be desired. One means to fix a soft 25 tissue to the selected area is to provide a suture through a selected portion of the soft tissue and fix the other end of the suture to a selected area on the bone with the fastener. To secure the sutures, the free ends of the suture are tied together to form a knot.

The use of knots in surgical procedures, however, can be improved upon. In minimally invasive procedures, such as arthroscopic or laparoscopic procedures, the surgical site is not readily accessible and limits the surgeon's ability to tie a knot manually. One remote method of securing the suture 35 6; is tying each of the suture ends into a knot extracorporeally and then remotely advancing the knot into the surgical site using suitably configured instruments. Securing the suture remotely can be cumbersome and time-consuming.

Accordingly, there is a need for improved devices for 40 securing a suture without a knot. There is a need for surgical methods to facilitate easy and efficient securing of the suture.

SUMMARY

The present teachings provide methods of attaching a soft tissue to an adjacent bone at a defect site. An adjustable loop of a flexible construct contained in a bore defined by a fastener is passed through the soft tissue. The fastener is 50 passed back through the adjustable loop to fold the adjustable loop upon itself. The fastener is attached to the bone. An adjusting arm on the flexible construct is engaged to reduce the size of the adjustable loop and secure the soft tissue to the bone.

The present teachings also provide methods of repairing a cartilage defect. An adjustable loop of a flexible construct is offset through a bore defined by a fastener. The adjustable loop is secured to a proximal end of the fastener with a restriction element. The adjustable loop is passed through the cartilage. The fastener is passed back through the adjustable loop to fold the adjustable loop upon itself. The fastener is fixed to an area adjacent the cartilage defect such that the adjustable loop and a proximal end of the fastener abut the cartilage defect. An adjusting arm on the flexible construct 65 is engaged to reduce the size of the adjustable loop and secure the soft tissue to the bone.

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The present teachings further provide methods of attaching a soft tissue to an adjacent bone at a defect site. An adjustable loop of a first flexible construct contained in a bore defined by a first fastener is passed through a tissue.

The first fastener is then attached to the bone. A second fastener having a second adjustable loop of a second flexible construct passed through a bore therein is passed through the first adjustable loop on the first fastener. The second fastener is passed back through the first adjustable loop to interlace the first adjustable loop and the second adjustable loop.

Further areas of applicability will become apparent from the description provided herein. It should be understood that the description and specific examples are intended for purposes of illustration only and are not intended to limit the scope of the present disclosure.

DRAWINGS

The drawings described herein are for illustration purposes only and are not intended to limit the scope of the present disclosure in any way.

FIG. 1 depicts a flexible construct according to various embodiments;

FIG. 2 depicts a fully extended flexible construct according to various embodiments;

FIGS. 3A and 3B depict movement of the adjustable loop according to various embodiments;

FIG. 4 depicts an assembly of an adjustable loop disposed about a suture anchor according to various embodiments;

FIG. 5 depicts a cross-section of the assembly of FIG. 4; FIG. 6 depicts the adjustable loop disposed about a suture anchor and attached to a driver according to various embodiments;

FIG. 7 depicts an exploded view of the assembly of FIG.

FIGS. 8A through 8E depict a surgical technique according to various embodiments; and

FIGS. 9A through 9D depict a surgical technique using two flexible constructs according to various embodiments.

DETAILED DESCRIPTION

The following description is merely exemplary in nature and is not intended to limit the present disclosure, application, or uses. Although certain examples and surgical methods disclosed herein are in conjunction with a suture anchor, it is understood that the suture fixation device can be any device with which to hold a suture. While the present teachings are disclosed in connection with labral repairs, it is understood that the devices and surgical techniques can easily be adapted for other orthopedic and non-orthopedic uses.

Referring to FIGS. 1 through 3B, the flexible construct 10 includes an adjustable loop 12, a passage 14, and an adjusting arm 16. Reduction of the adjustable loop 12 compresses the tissue and provides fixation of the tissue. The adjustable loop 12 and the surgical methods detailed herein, eliminate the need to tie a knot and thereby increase surgical efficiency. As compared to traditional sutures secured by tying a knot, the flexible construct 10 of various embodiments provides increased load to failure, has multiple-fold increased strength, has a decreased stretch at failure, and has multiple-fold stiffness at failure.

Referring to FIG. 2, the flexible construct 10 can be made from any biocompatible material that is flexible and can pass through and secure a tissue. Exemplary materials include, but are not limited to, non-resorbable polymers, such as

polyethylene or polyester, resorbable polymers, metals, and various combinations thereof. The materials can include those formed into a monofilament, multiple filaments, cables, and the like. In various embodiments, the flexible construct 10 is made of a hollow material to allow for the 5 appropriate folding and tensioning thereon.

In various embodiments, the flexible construct 10 can be a suture 18. The suture 18 used to form the construct is generally a hollow suture having a distal end 20 and proximal end 22. The suture 18 can be formed as a braided or 10 multiple-filament suture structure that is formed to define a substantially tubular hollow-shaped flexible construct 10.

The suture 18 contains a first opening 24 located closer to the distal end 20 and the second opening 26 located closer to the proximal end 22. In various embodiments, the first opening 24 and the second opening 26 can extend along a top surface of the suture 18 and are sized to accommodate passage of the distal end 20 of the suture therethrough. It is understood that the first opening 24 and the second opening 26 need not be formed by cutting the suture 18 or by removing any suture material. For example, the first opening 24 or the second opening 26 can be formed by passing the suture distal end 20 through the sidewall of the hollow tubular suture 18.

alloys of cobalt, chromium polyetheretherketone (PEEI of lactic and glycolic acid.

At the distal end of anch substantially ease entry of the into the bone portion. The pointed as shown in FIGS anchor 100 such that the apprediction provided as shown in FIGS anchor 100 such that the apprediction in a honey thereto without damaging the ments, the asymmetric suture

The passage 14 is defined by the area between the first 25 opening 24 and the second opening 26. The passage 14 can be a short passage, can extend to the length of a fastener used therewith, or have a greater length, as further detailed later herein.

To provide the adjustable loop 12 and the adjusting arm 30 16, the distal end 20 of the suture 18 is passed through the first opening 24, into and through the passage 14, and advanced out of the second opening 26. The portion exiting from the second opening 26 provides the adjusting arm 16 and the folded end provides the adjustable loop 12.

Other adjustable loops that are useful in the various embodiments detailed herein are disclosed in U.S. patent application Ser. No. 11/541,506 to Stone, filed Sep. 29, 2006, and assigned to Biomet Sports Medicine, Inc., which is hereby incorporated by reference.

Referring to FIGS. 3A and 3B, the adjusting arm 16 is engaged or pulled in direction A to cause movement of the adjustable loop 12. As the adjustable loop 12 is reduced in size (or creating a smaller diameter loop 12), the adjusting arm 16 lengthens as shown in FIG. 3B, In various embodiments, the movement of the suture 18 is only in the direction of arrow A and movement is prevented in the opposite direction. This unidirectional movement is controlled by maintaining tension (by pulling, for example) on the flexible construct 10 to radially compress the passage 14 about the 50 suture portion contained therein as further detailed later herein.

To facilitate the unidirectional movement, a restriction element 28 can be included near the proximal end 22. The restriction element 28 controls movement of the adjustable 55 loop 12 and the adjusting arm 16. Moreover, the restriction element 28 can prevent displacement of the flexible construct 10 in minimally invasive procedures. As depicted, the restriction element 28 is a knot. It is understood that the restriction element 28 does not provide the tissue fixation, 60 but it is the tissue compression provided by the reduction of the adjustable loop 12 about the tissue that provides the fixation. The restriction element 28 can include other devices used to retain a suture, such as a suture clip.

The flexible construct 10 can be attached to a fastener to 65 create an assembly. As shown in FIGS. 4 and 5, an asymmetric suture anchor 100 is used as the fastener. The

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asymmetric suture anchor 100 is similar to anchors described in U.S. patent application Ser. No. 11/386,068 to Stone et al., filed Mar. 21, 2006, and assigned to Biomet Sports Medicine, Inc., which is hereby incorporated by reference.

The asymmetric suture anchor 100 includes a tip 102, an anchor body 104 having an interior bore 106, an exterior suture-receiving channel 108 defined by one side of the anchor body, and a port 110 connecting the interior bore 106 and the exterior suture-receiving channel 108. The anchor can be made of any biocompatible material including, but not limited to, a metal, such as titanium, stainless steel, or alloys of cobalt, chromium, etc., or a polymer such as polyetheretherketone (PEEK) or polymers and copolymers of lactic and glycolic acid.

At the distal end of anchor 100, the tip 102 is adapted to substantially ease entry of the asymmetric suture anchor 100 into the bone portion. The tip 102 can be generally smooth or rounded as shown in FIGS. 4 and 5, or the tip 102 can be pointed as shown in FIGS. 6-9D. The tip 102 guides the anchor 100 such that the anchor 100 can be placed into a pre-drilled hole in a honey tissue to reattach a soft tissue thereto without damaging the soft tissue. In various embodiments, the asymmetric suture anchor 100 can be rotated or twisted upon insertion into the pre-drilled hole to align and set the asymmetric suture anchor 100 prior to completely advancing the anchor 100 to its final position.

Attached to the tip 102 is the anchor body 104. The anchor body 104 can be externally threaded or have helical or annular ribs. The threading can be a helical thread which starts at the meeting point of the tip 102 and the anchor body 104 as shown in threads 112. The threads 112 facilitate engagement of the tissue by the asymmetric suture anchor 100.

A bore 106 in the anchor body 104 extends from a proximal end of the anchor body 104 through an interior portion of the anchor body. The bore 106 generally extends along the longitudinal axis of the anchor body 104 and is open at the proximal end. The bore 106 can be offset with the outer diameter of the anchor body or the bore 106 can be concentric with the outer diameter of the anchor body. The bore 106 provides an area in which a region of the adjustable loop 12 can be placed in the interior of the anchor body 104. The bore 106 is sufficiently sized to prevent passage of the restriction element 28 therethrough. Generally, the restriction element 28 is larger than the bore 106 and cannot fit therein.

As shown in FIG. 5, the restriction element 28 can optionally be connected to the adjustable loop 12 to further secure the adjustable loop 12 in the anchor 100. In such embodiments, the restriction element 28 can be attached to the adjusting arm 16. The adjusting arm 16 can be sewn or knotted into the restriction element to create a bridge or passage across the proximal end of the anchor 100. The adjusting arm 16 can also be passed through the adjustable loop 12 to interlace the adjusting arm 16 and the adjustable loop 12. In either such embodiment, the adjustable loop is further secured to the anchor 100.

The bore 106 is connected to a suture-receiving channel 108 with the port 110. The suture-receiving channel 108 is located on an exterior surface of the anchor body 104. The suture-receiving channel 108 provides an area in which a region of the adjustable loop 12 can optionally be placed on the exterior of the anchor body 104 without damaging the flexible construct 10.

The port 110 connecting the suture-receiving channel 108 and the interior bore 106 is generally perpendicular to at

least one of the suture-receiving channel 108 and the interior bore 106. The port 110 provides the communication between the inside of the anchor (interior bore 106) and the outside of the anchor (suture-receiving channel 108). The port 110 is sized to receive the adjustable loop 12. As shown, the port 110 and the external suture-receiving channel 108 partially extend into the tip 102 and provide a break in the threading 112. The port 110 can have the same diameter as the interior bore 106. In various embodiments, the port 110 diameter, the interior bore 106 diameter, and the cross-section of the 10 suture-receiving channel 108 are the same. The anchor 100 is stable and will not toggle when stress is placed on the anchor 100.

The suture-receiving channel 108 and the bore 106 are considered to be offset or asymmetrical due to the adjustable 15 loop 12 being partly received in the interior of the anchor body 104 at the bore 106 and partly received in the exterior of the anchor body 104 at the suture-receiving channel 108. The combination and arrangement of the bore 106, the suture-receiving channel 108, and the port 110 form a 20 continuous track or loop around which the adjustable loop 12 can be wrapped. In various embodiments, the passage 14 can be sized to be longer than the track or loop. This allows for radially compression or tensioning of the passage 14 using the anchor 100 and thereby prevents movement of the 25 adjustable loop 12.

The asymmetric suture anchor 100 can include a proximal end groove 114 to receive the suture and provides a surface upon which the restriction element 28 abuts. The proximal end groove 114 is in communication with the opening at the 30 proximal end of the anchor body 104.

The proximal end of the asymmetric suture anchor 100 also includes a driver-engaging region 116, such as those detailed earlier herein. Particular to the asymmetric anchor, the proximal end groove 114 can be provided with a key 118, 35 depicted as inwardly curving shapes which will be axially received in the mating female driver.

Although the various embodiments detailed herein are used in connection with the asymmetric suture anchor 100, it is understood that any other anchor or screw can be used 40 in connection with the adjustable loop 12. Suitable anchors can include an interior bore or opening in which to house the adjustable loop 12 and/or include features to protect the flexible construct 10.

Referring to FIGS. 6 and 7, the anchor 100 and the 45 adjustable loop 12 combination is mated or connected to a driver 200. The driver 200 includes a handle 202, an adjusting arm receptacle 204, an adjustable loop mount 206, and an elongated, hollow shaft 208.

The handle 202 is located at the driver first proximal end 210. The handle 202 is partially hollow and is in communication with the shaft 208 at the shaft first proximal end 212 to facilitate passage of the adjusting arm 16 from the proximal end groove 114 of the anchor, down through the shaft 208, and out of the adjusting arm receptacle 204 on the 55 handle 202. The handle 202 further includes the adjustable loop mount 206 to secure the adjustable loop 12 such that advancement of the driver 200 having the anchor 100 thereon through the cannula does not unintentionally move the adjustable loop 12.

To connect the driver 200, the anchor 100, and the flexible construct 10, the adjustable loop 12 is passed through the bore 106 of the anchor 100. The restriction element 28 is arranged to contact the proximal end groove 114. The adjusting arm 16 is extended through the hollow shaft 208, 65 passed through the handle 202, and passed through the adjusting arm receptacle 204. The anchor 100 is oriented in

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close proximity to a second distal end 214 of the shaft 208. Next, the adjustable loop 12 is directed through the external suture-receiving channel 108 of the anchor 100 and out of the port 110. The driver-engaging feature 118 of the anchor 100 is then connected to the mated feature on the shaft second distal end 214. The adjustable loop 12 can be aligned adjacent to the exterior of the shaft 208 to extend the adjustable loop 12 to the adjustable loop mount 206. In embodiments employing a restriction element 28, the restriction element 28 can be sized to prevent passage of the restriction element through the shaft 208.

Next, the adjustable loop 12 can be removably fixed or connected to the adjustable loop mount 206. The adjustable loop mount 206 keeps the flexible construct 10 in proper alignment with the shaft 208 such that advancement of the driver 200 having the anchor 100 and flexible construct 10 thereon, through a cannula 216 does not unintentionally move the flexible construct 10. Attaching the adjustable loop 12 to the adjustable loop mount 206 provides compression of the passage 14 and thereby restricts movement of the adjustable loop 12 in the direction opposite to arrow A of FIGS. 3A and 3B. When the adjustable loop 12 is disengaged from the adjustable loop mount 206, moving the adjusting arm 16 causes a reduction in the size of the adjustable loop 12. In various embodiments, the adjustable loop 12 need not be mounted to the adjustable loop mount **206**.

The tension can be maintained on the adjusting arm 16 by containing the adjusting arm 16 in the adjusting arm receptacle 204 or by other suitable means. As long as tension is maintained on the adjusting arm 16 (for example, via the adjusting arm receptacle 204) and the adjustable loop 12 (for example, via the adjustable loop mount 206), the flexible construct 10 will not move while on the driver.

In various embodiments, the flexible construct 10 is used to fix a defect where there is a need to fix a soft tissue or implant to a bone. The flexible construct 10 and surgical techniques detailed herein can be used with various repairs of the shoulder, wrist, hand, ankle, foot, elbow, knee, or hip as non-limiting examples. Exemplary repairs include Bankart Repair, SLAP Repair, Acromioclavicular separation, rotator cuff repair, capsule repair or capsulolabral reconstruction, biceps tenodesis, or deltoid repair of the shoulder; scapholunate ligament reconstruction or ulnar radial collateral ligament reconstruction of the wrist or hand; lateral stabilization, medial stabilization, Achilles tendon repair and reconstruction, halux valgus reconstruction, midfoot reconstruction, and forefoot reconstruction of the ankle or foot; lateral epicondylitis (tennis elbow) repair, ulnar or radial collateral ligament reconstruction, and biceps tendon reconstruction of the elbow; and extra-capsular repair, medial collateral ligament repair, lateral collateral ligament repair, posterior oblique ligament repair, joint capsule closure, iliotibial band tenodesis reconstruction, patellar realignment and repair, patellar ligament and tendon repair, and vastus medialis obliquus muscle advancement.

Referring to FIGS. 8A through 8D, methods of repairing a soft tissue defect, such as a cartilage defect are provided. The adjustable loop 12 is offset in the bore 106 of the asymmetric suture anchor 100 and affixed to the driver 200 as detailed above. The adjustable loop 12 is released from the adjustable loop mount 206, if used, and the assembly is placed in the cannula 216 at the defect site 300.

The adjustable loop 12 is then passed through the cartilage 302 as shown in FIG. 8B. The adjustable loop 12 can be passed through the cartilage 302 by piercing a hole in the cartilage prior to passing the suture therethrough. This can

be performed with a separate needle, a needle that is removably attached to the adjustable suture loop 12 or, depending on the fastener used, with a tip of the fastener. Any suitable suture passer or other device can also be used to pass the adjustable loop 12 through the cartilage 302 such as those known in the art as "bird beak" passers or suture lariats. Two devices useful for passing the suture include those sold under the tradenames SpeedPass and ArthroPass, both made by Biomet Sports Medicine, Inc. of Warsaw, Ind. A front portion 30 of the adjustable loop is passed through and protrudes from the cartilage 302.

The front portion 30 is lengthened (or further pulled through the cartilage 302) to provide an area in which to fold the adjustable loop 12 upon itself. The front portion 30 is wrapped around the anchor 100 to form an S-shape which spans between the tissue and the anchor 100. The anchor 100 is then passed back through the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 12 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 13 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 14 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 15 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 15 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 15 as shown in FIG. 8C. This wrapping or doubling of the adjustable loop 15 as shown in FIG. 8C. Thi

The anchor 100 is then placed in a pre-drilled hole 304 in an adjacent bone 306 as shown in FIG. 8D. The threads 112 secure the anchor 100 in the bone hole 304. The driver 200 can be removed once the anchor 100 is secured in the bone 306. This can be performed prior to or after the suture is 25 tightened down against the tissue.

Next, the adjusting arm 16 is engaged to reduce the size of the adjustable loop 12. The restriction element 28 keeps the adjustable loop 12 in place on the anchor 100 and prevents retreat of the adjustable loop 12 through the shaft 30 208. When the adjusting arm 16 is advanced sufficiently far to provide the appropriate compression to the cartilage 302 and fix the cartilage 302 at the defect site 300, the ends of the adjusting arm 16 can be removed as shown in FIG. 8E.

At least a portion of the proximal end of the anchor 100 is in very close proximity to the cartilage 302 or abuts the cartilage 302, thereby enhancing the fixation of the cartilage 302 to the bone 306. In various embodiments, the suture-receiving channel 108 of the anchor can abut the cartilage 302 to minimize the length of suture 18 that remains 40 between the beginning of the available or suturable suture in the bone hole 304 and the cartilage 302 or the other tissue to be secured. When the offset or channel 108 area of the anchor body 104 abuts the defect site 300, the repair is stronger due to the ability to more tightly secure the tissue 45 to the underlying bone 306 and the ability to minimize the gap or lag between the anchor body 104 and the tissue.

Such embodiments where the proximity between the tissue and the anchor 100 is optimized are particularly useful in repairing certain soft tissue defects, for example, a labral 50 tear. The anchor body proximal end would abut the labrum and provide strong attachment and promote healing of the labral tear and restore strength to the shoulder or the hip, for example.

The above-mentioned repair techniques can be used for 55 any orthopedic repair including cartilage repair, ligament repair, or tendon repair, or any other orthopedic repair. The repair can be with an articular orthopedic surface or a non-articular and/or non-orthopedic surface.

Referring to FIGS. 9A through 9D, the present teachings 60 also provide surgical methods where multiple flexible constructs 10 and 10' are incorporated with multiple suture anchors 100 and 100'. To start, a first anchor 100 is inserted as described above herein. Prior to removing the first shaft 208 of the first driver 200, the second loop 12' is passed over 65 the first shaft 208 as shown in FIG. 9A. Next, the first shaft 208 and the first driver 200 are then removed from the defect

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site 300. The second anchor 100' is then passed through the first loop 12 again to interlace the adjustable loops 12 and 12' as shown in FIG. 9B.

The second anchor 100' is then secured through the tissue 302 and into the bone 306. The first adjusting arm 16 and the second adjusting arm 16' are then engaged to cause the respective loops to reduce in size and form a link or bridge 400 of interlaced adjustable loops 12 and 12' between the first anchor 100 and the second anchor 100'. After the adjusting arms 16 and 16' are engaged to the correct distance to reduce the respective adjustable loops and provide the appropriate amount of tissue compression and securing at the defect site 300, the adjusting arms 16 and 16' can be optionally cut. There is no need for the surgeon to tie a knot as the interlaced and compressed loops provide the tissue fixation.

These surgical methods can be expanded to include a plurality of adjustable loops and a plurality of suture anchors. In such embodiments, the anchors are inserted in succession as detailed above. Each subsequent anchor is then wrapped through the adjustable loop of any prior anchor and then inserted into the tissue. The respective adjusting arms are then engaged advanced to create a larger interlaced bridge system.

The description of the present teachings is merely exemplary in nature and, thus, variations that do not depart from the gist of the present teachings are intended to be within the scope of the present teachings. Such variations are not to be regarded as a departure from the spirit and scope of the present teachings.

What is claimed is:

1. A suture anchor assembly, comprising:

an anchor for insertion into a hole in a bone, the anchor having a longitudinal axis that extends between a proximal end and a distal end of the anchor, the anchor including a first opening in the proximal end of the anchor which leads to a longitudinal interior bore in the anchor, the anchor further including a second opening in a side wall of the anchor which leads to a transverse passage in the anchor, the transverse passage proximate the distal end of the anchor and connecting the longitudinal interior bore in the anchor to a longitudinal exterior channel in the anchor that extends along an outer surface of the anchor; and

an adjustable suture construct that includes a suture with a first free end that passes through a first longitudinal passage in the suture to form a first adjustable loop, wherein the adjustable suture construct is coupled to the anchor such that the first longitudinal passage in the suture: (i) extends along the longitudinal interior bore; (ii) passes through the transverse passage; (iii) exits the anchor through the second opening in the side wall of the anchor; and (iv) extends along the outer surface of the anchor in the longitudinal exterior channel in the anchor,

wherein the first longitudinal passage in the suture protrudes from the second opening in the side wall of the anchor such that the first adjustable loop extends away from the second opening.

- 2. The suture anchor assembly of claim 1, wherein the first longitudinal passage in the suture extends along the entirety of the longitudinal interior bore in the anchor.
- 3. The suture anchor assembly of claim 1 further comprising a driver carrying the anchor.
- 4. The suture anchor assembly of claim 3, wherein the driver includes an adjustable loop mount to which the first adjustable loop is removeably fixed.

- 5. The suture anchor assembly of claim 4, wherein the first adjustable loop being removeably fixed to the adjustable loop mount includes a portion of the first adjustable loop being positioned around the adjustable loop mount.
- 6. The suture anchor assembly of claim 1, wherein the entirety of the first adjustable loop is positioned outside the anchor.
- 7. The suture anchor assembly of claim 1, wherein at least part of the first adjustable loop is positioned along the outer surface of the anchor in the longitudinal exterior channel in the anchor.
- 8. The suture anchor assembly of claim 1, wherein the first free end of the suture extends away from the first opening in the proximal end of the anchor.
 - 9. A suture anchor assembly, comprising:
 - an anchor for insertion into a hole in a bone, the anchor having a longitudinal axis that extends between a proximal end and a distal end of the anchor, the anchor including a first opening in the proximal end of the anchor which leads to a longitudinal interior bore in the 20 anchor, the anchor further including a second opening in a side wall of the anchor which leads to a transverse passage in the anchor, the transverse passage proximate the distal end of the anchor and connecting the longitudinal interior bore in the anchor to a longitudinal 25 exterior channel in the anchor that extends along an outer surface of the anchor; and
 - an adjustable suture construct coupled to the anchor, the adjustable suture construct including a suture with a first free end that passes through a first longitudinal 30 passage in the suture to form a first adjustable loop,

wherein the adjustable suture construct being coupled to the anchor includes the adjustable suture construct 10

extending through the longitudinal interior bore in the anchor with the first adjustable loop extending away from the second opening in the side wall of the anchor and with the first free end of the suture extending away from the first opening in the proximal end of the anchor such that the first free end can be pulled to a reduce a size of the first adjustable loop,

wherein the first longitudinal passage in the suture protrudes from the second opening in the side wall of the anchor with at least part of the first adjustable loop being positioned along the outer surface of the anchor in the longitudinal exterior channel in the anchor.

- 10. The suture anchor assembly of claim 9, wherein the entirety of the first adjustable loop is positioned outside the anchor.
- 11. The suture anchor assembly of claim 9, wherein the first longitudinal passage in the suture extends along the entirety of the longitudinal interior bore in the anchor.
- 12. The suture anchor assembly of claim 11, wherein the first longitudinal passage in the suture: (i) extends along the longitudinal interior bore; (ii) passes through the transverse passage; (iii) exits the anchor through the second opening in the side wall of the anchor; and (iv) extends along the outer surface of the anchor in the longitudinal exterior channel in the anchor.
- 13. The suture anchor assembly of claim 9 further comprising a driver carrying the anchor.
- 14. The suture anchor assembly of claim 13, wherein the driver includes an adjustable loop mount to which the first adjustable loop is removeably fixed.

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