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Davison et al.

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(54) **VOLAR DISTAL RADIUS STABILIZATION SYSTEM**

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(51) **Int. Cl.**
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(52) **U.S. Cl.**
CPC *A61B 17/8085* (2013.01); *A61B 17/0401* (2013.01); *A61B 17/1728* (2013.01);
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(58) **Field of Classification Search**
CPC A61B 17/8085; A61B 17/80
See application file for complete search history.

(73) Assignee: **Globus Medical, Inc.**, Audubon, PA (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 203 days.

This patent is subject to a terminal disclaimer.

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(65) **Prior Publication Data**
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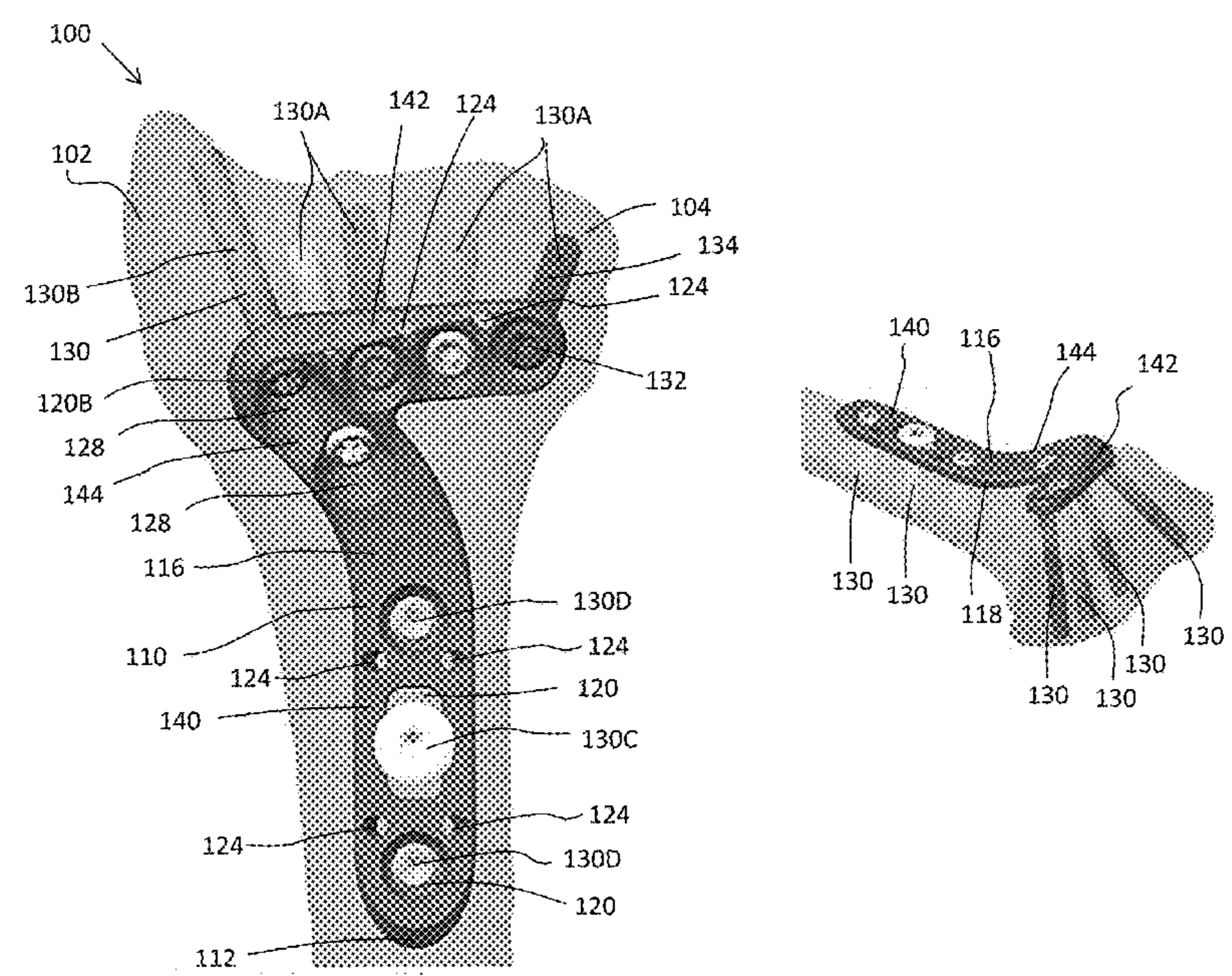
(57) **ABSTRACT**

Devices, systems, and methods for bone stabilization, especially volar distal radius stabilization. The stabilization system may include a bone plate having an elongated portion, an enlarged head portion, and a transition region connecting the elongated portion to the enlarged head portion, and the plate including a plurality of through holes. A plurality of fasteners may be configured to extend through one or more of the plurality of through holes in the bone plate and into the bone. The plate may be used to stabilize a fracture in a long bone, such as a radius.

Related U.S. Application Data

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14 Claims, 27 Drawing Sheets



Related U.S. Application Data

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A61B 17/04 (2006.01)
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(52) **U.S. Cl.**

CPC *A61B 17/1782* (2016.11); *A61B 17/80*
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17/809 (2013.01); *A61B 17/8014* (2013.01);
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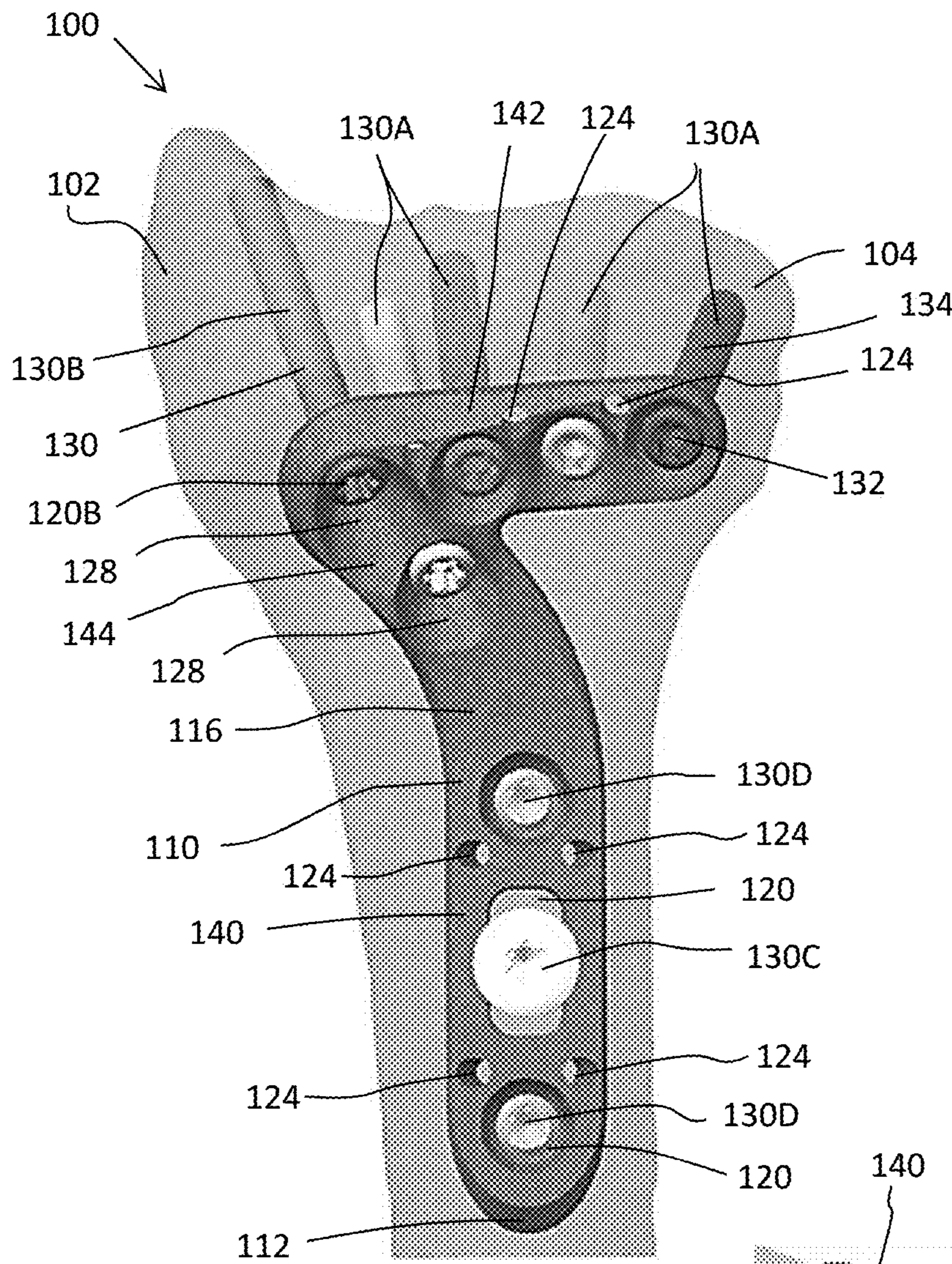


FIG. 1A

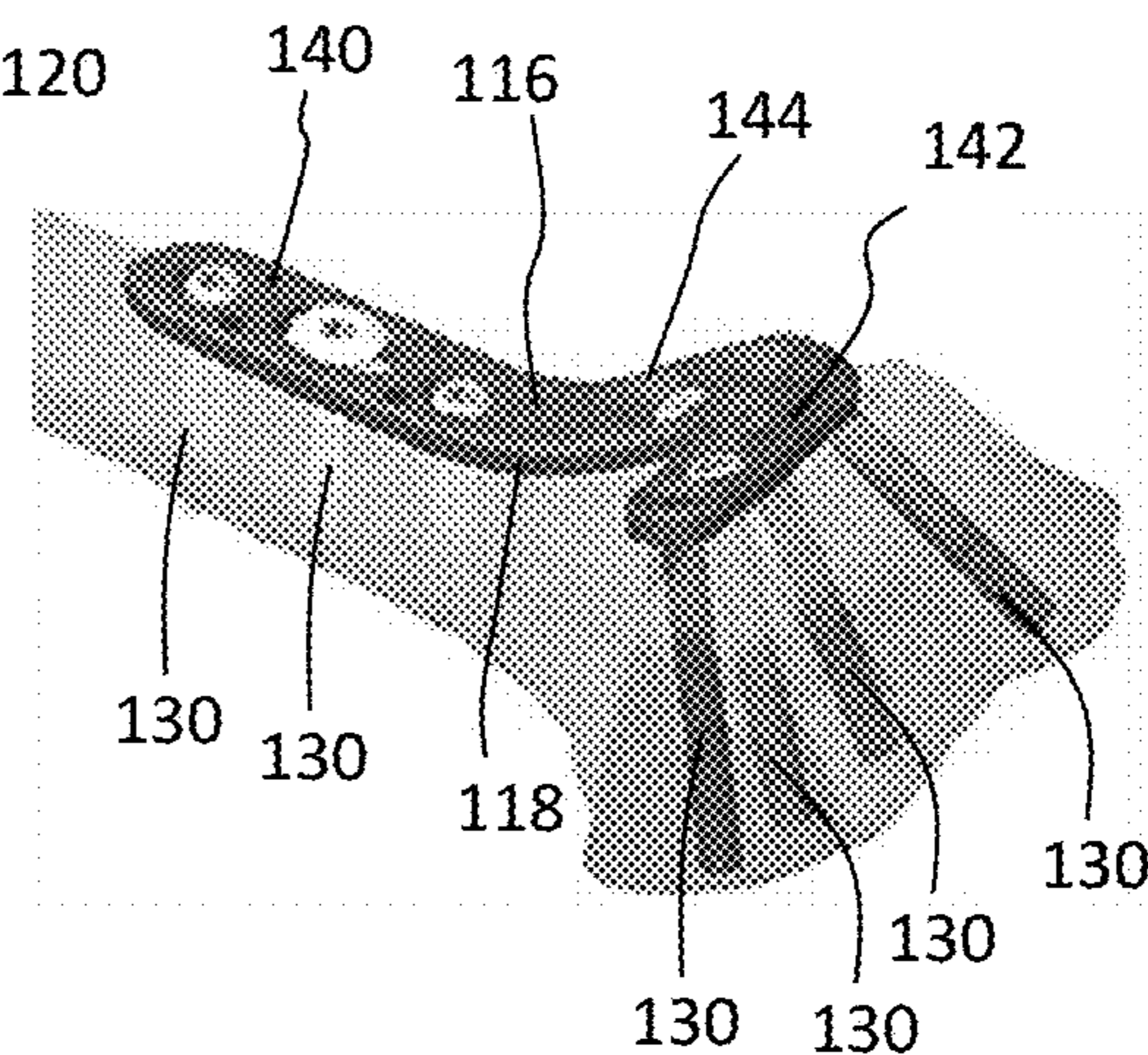
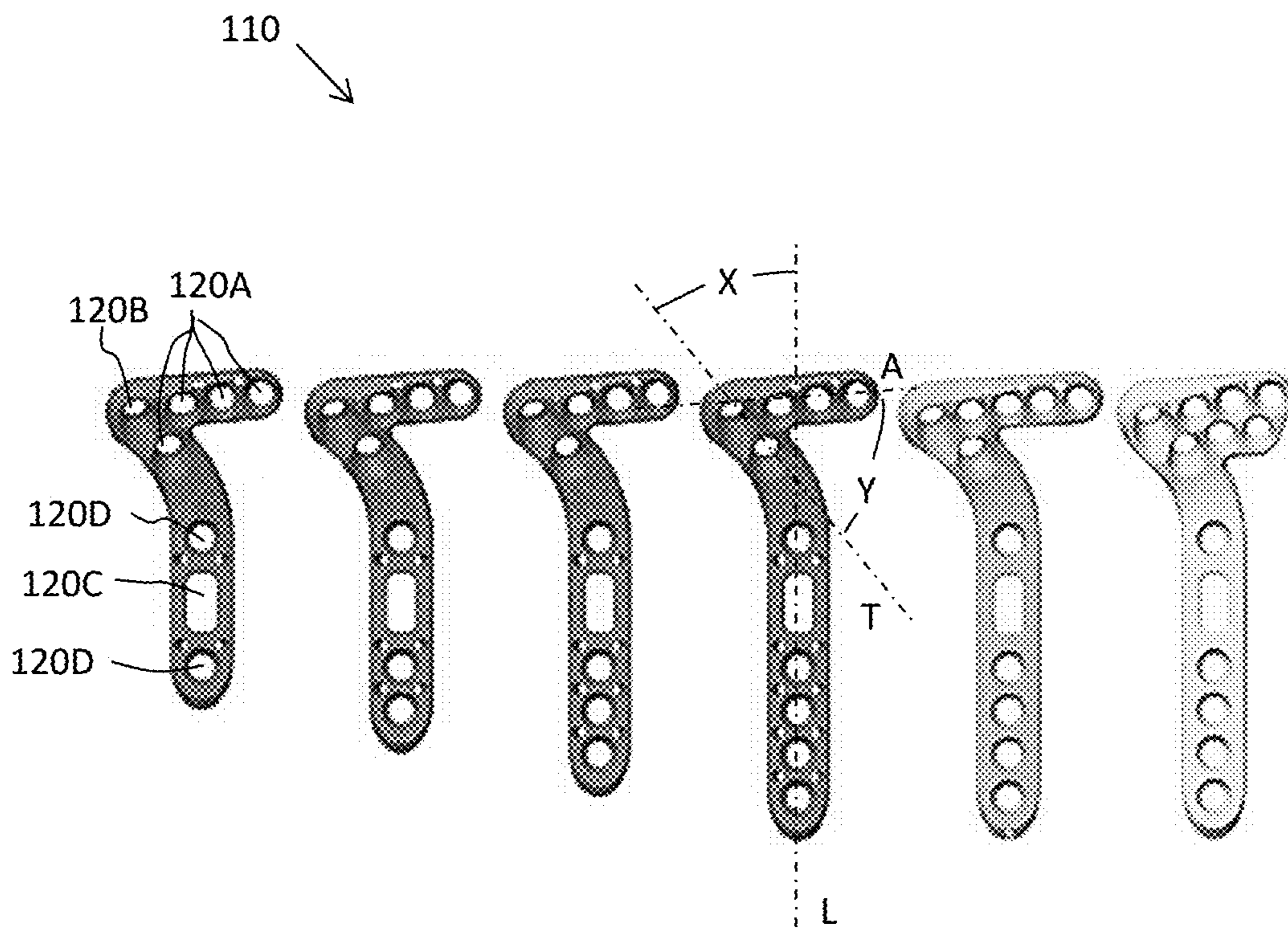


FIG. 1B



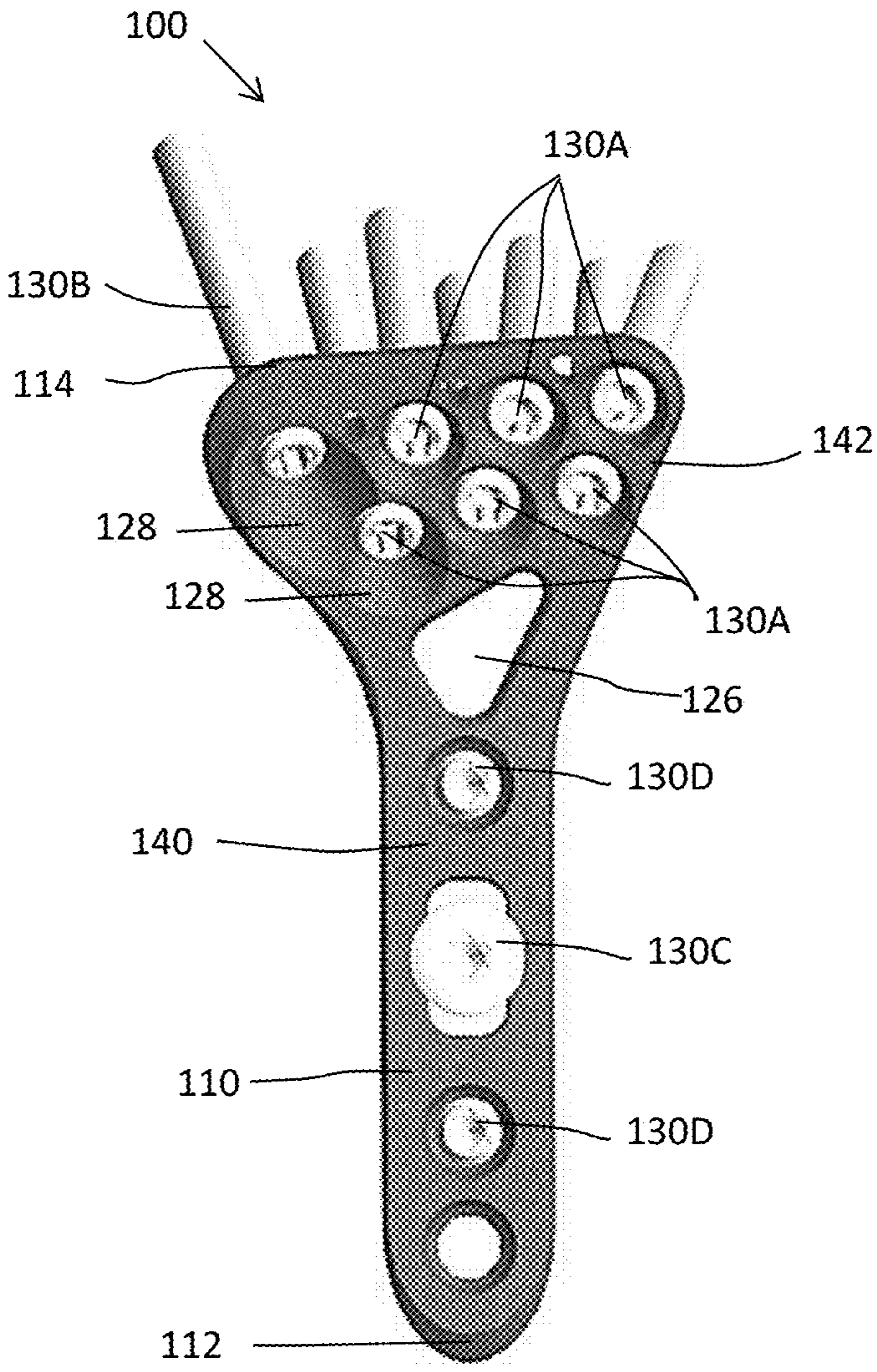


FIG. 1D

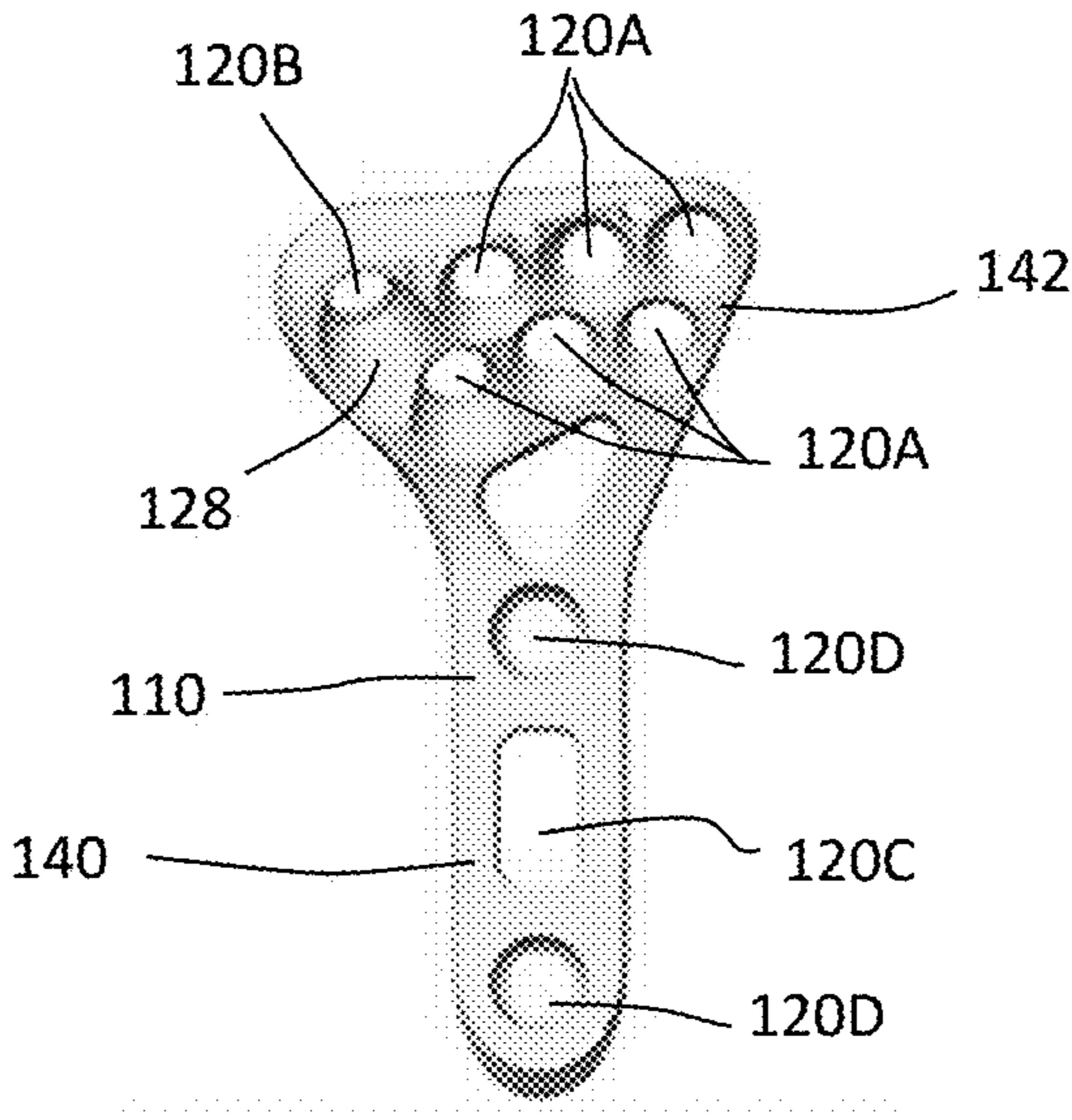


FIG. 1E

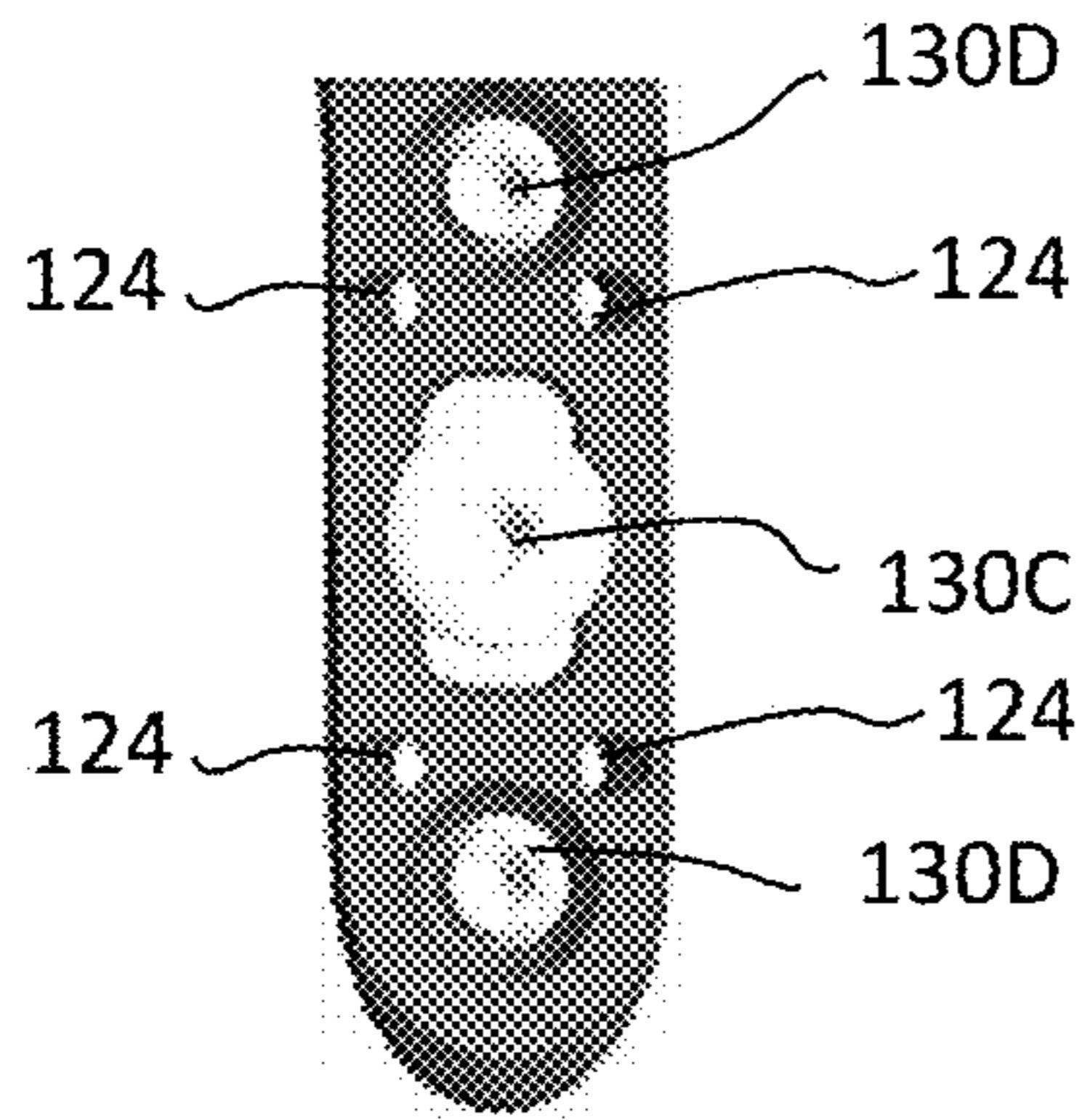


FIG. 1F

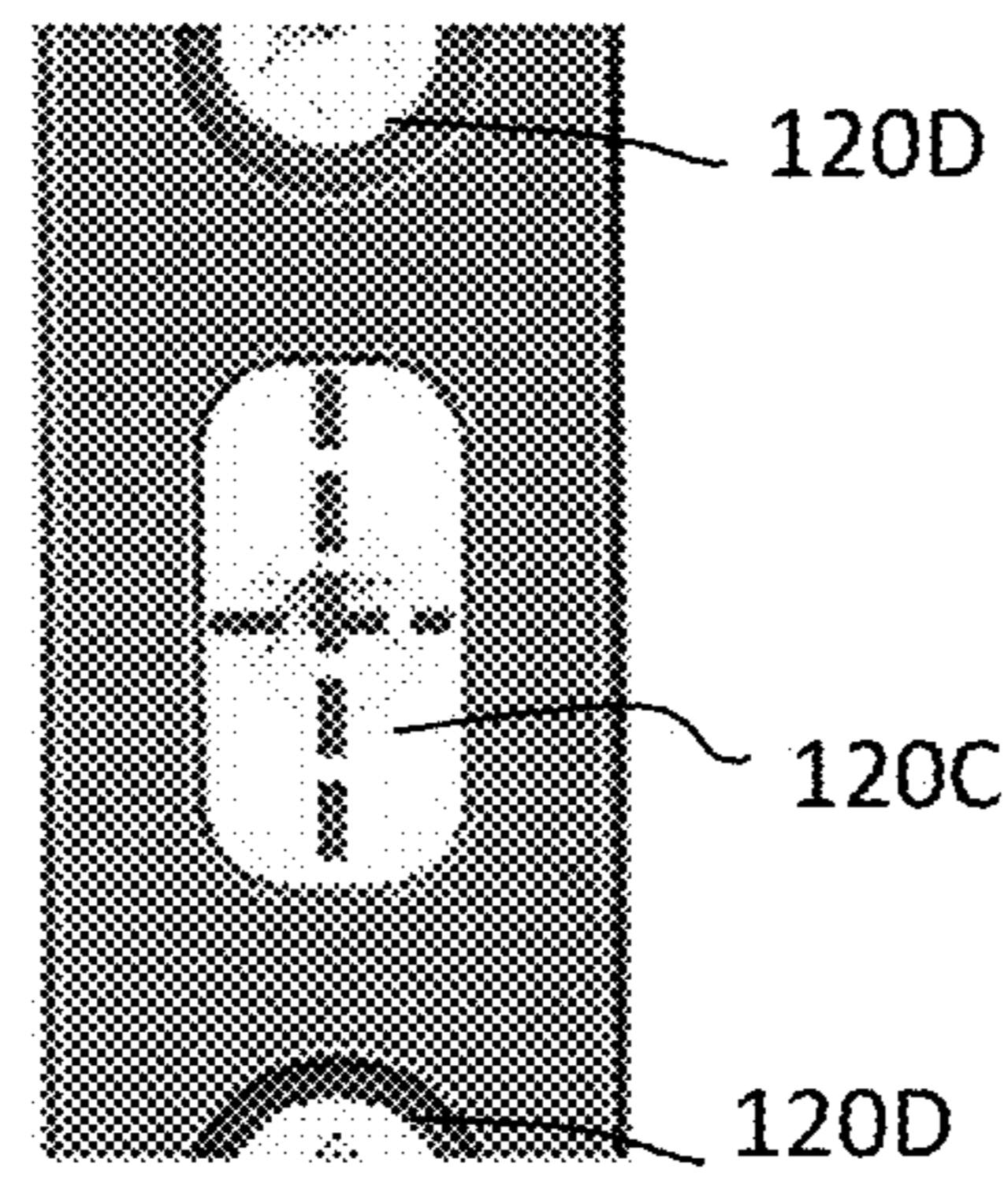


FIG. 1G

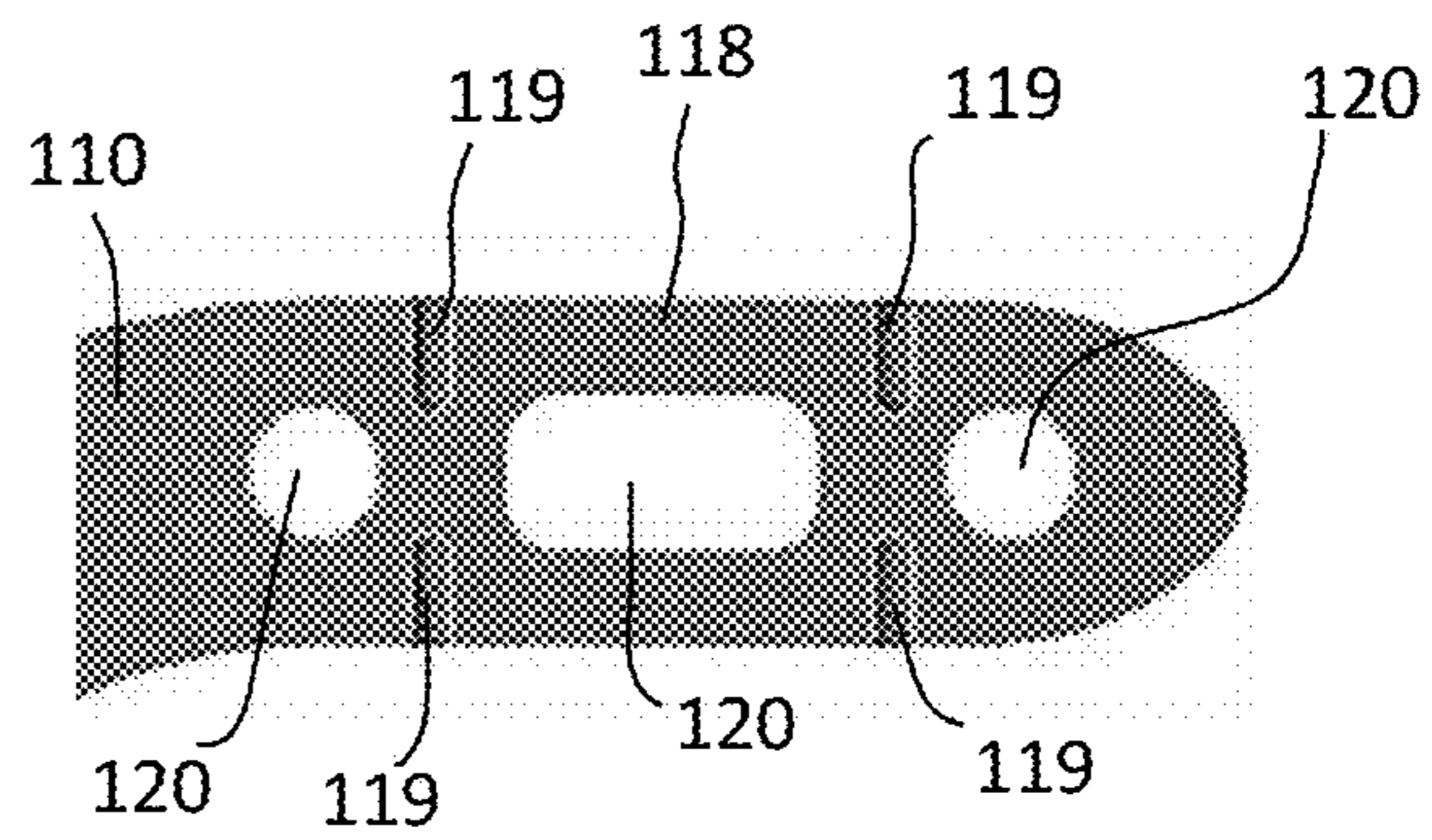


FIG. 1H

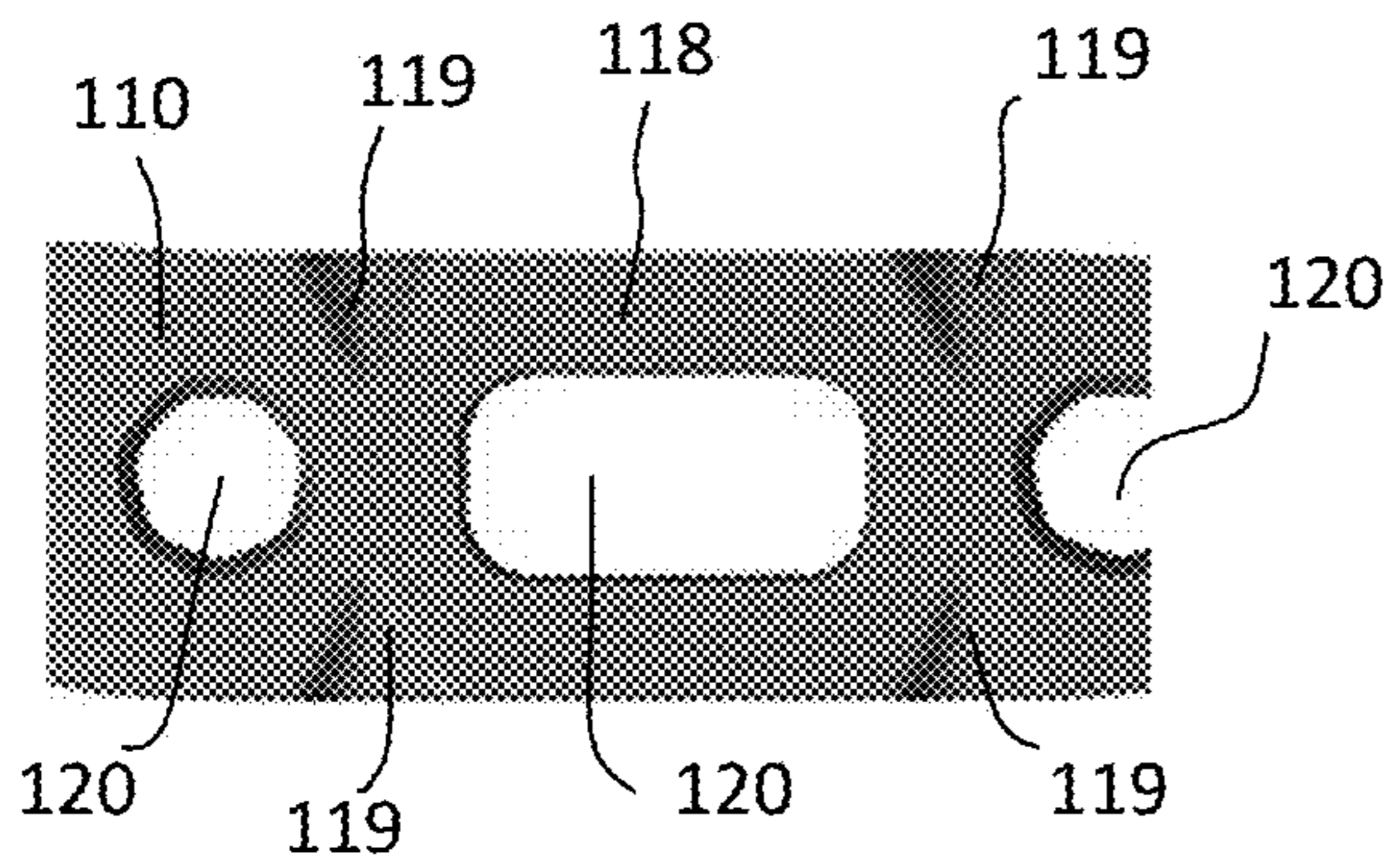


FIG. 1I

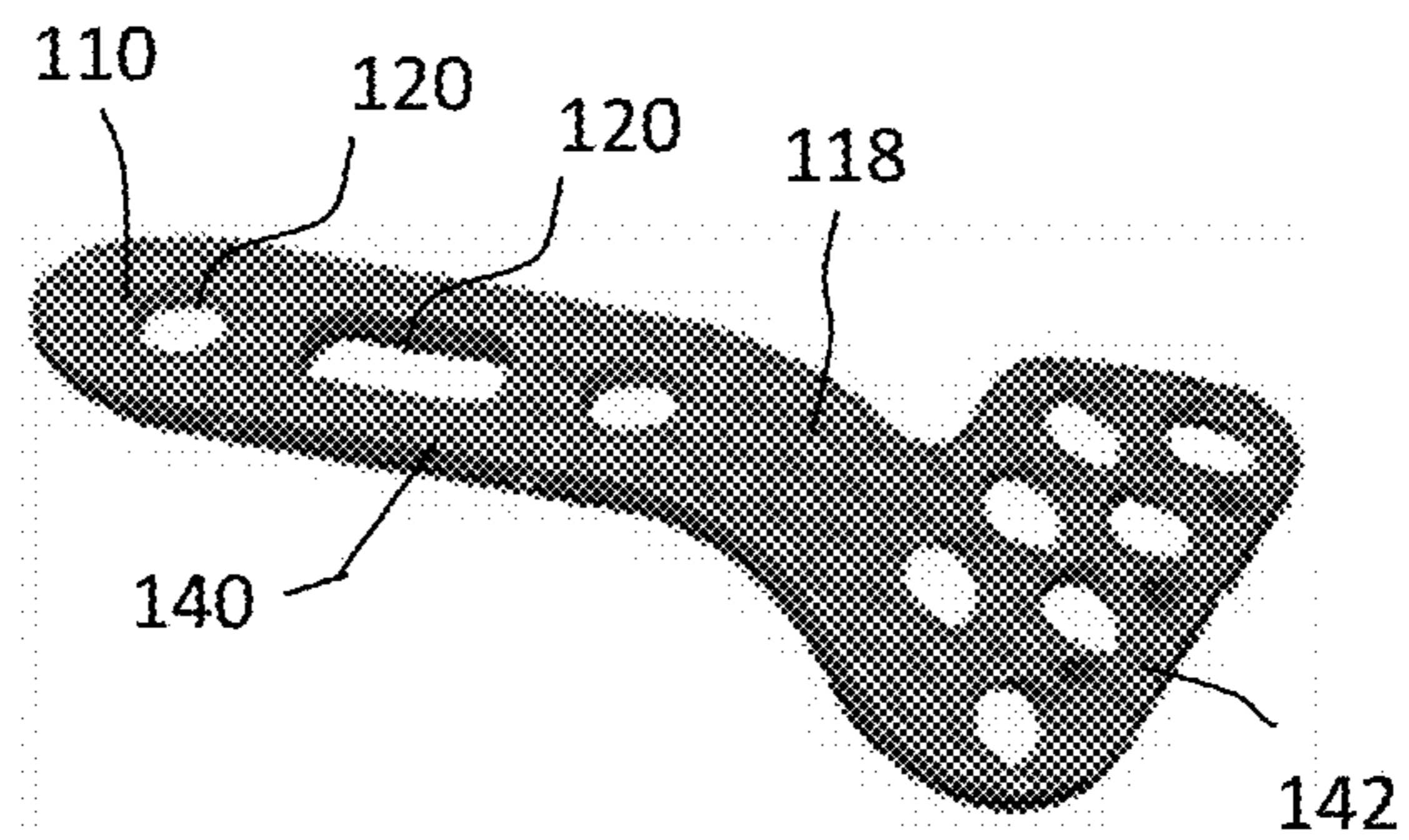


FIG. 1J

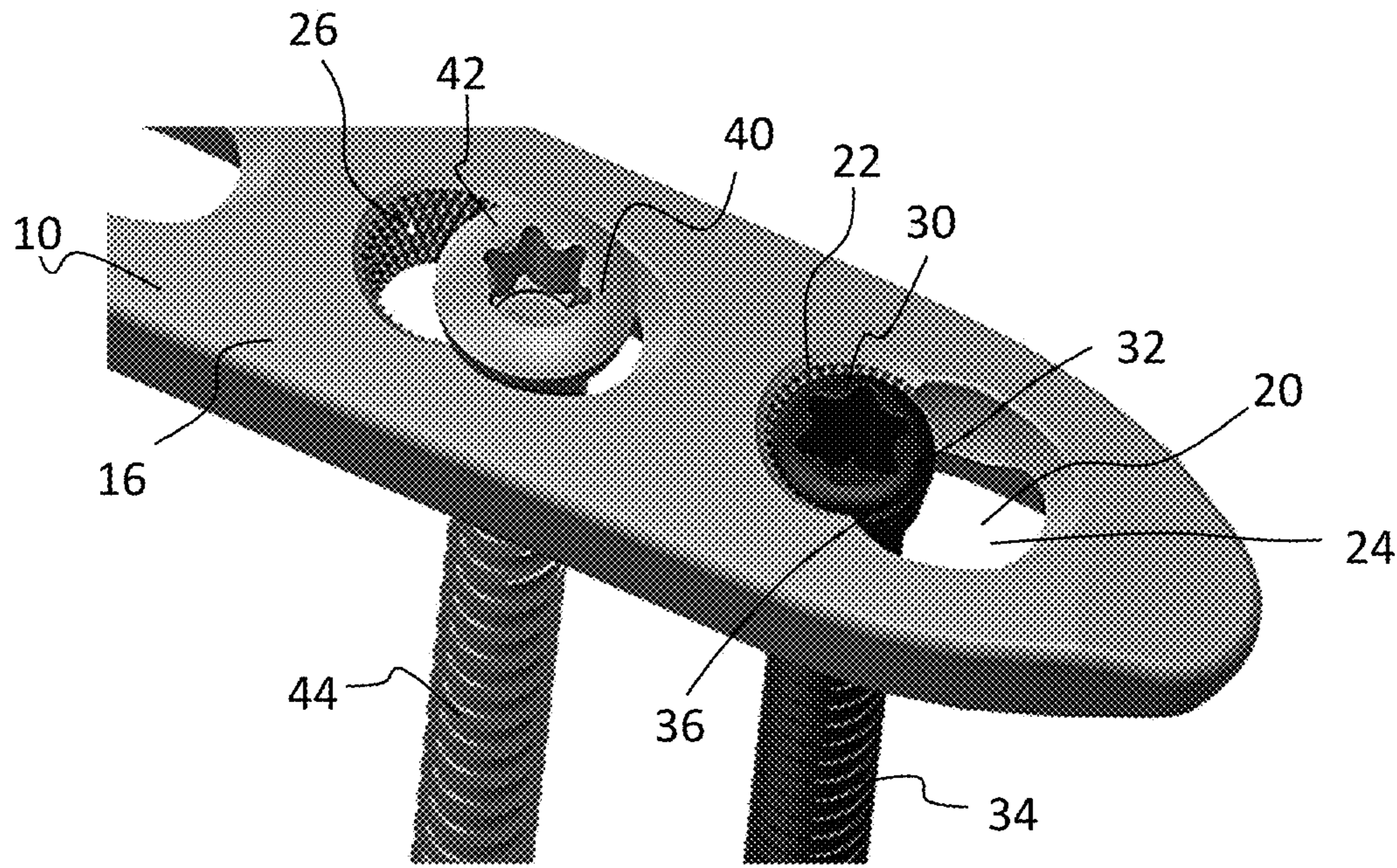


FIG. 2

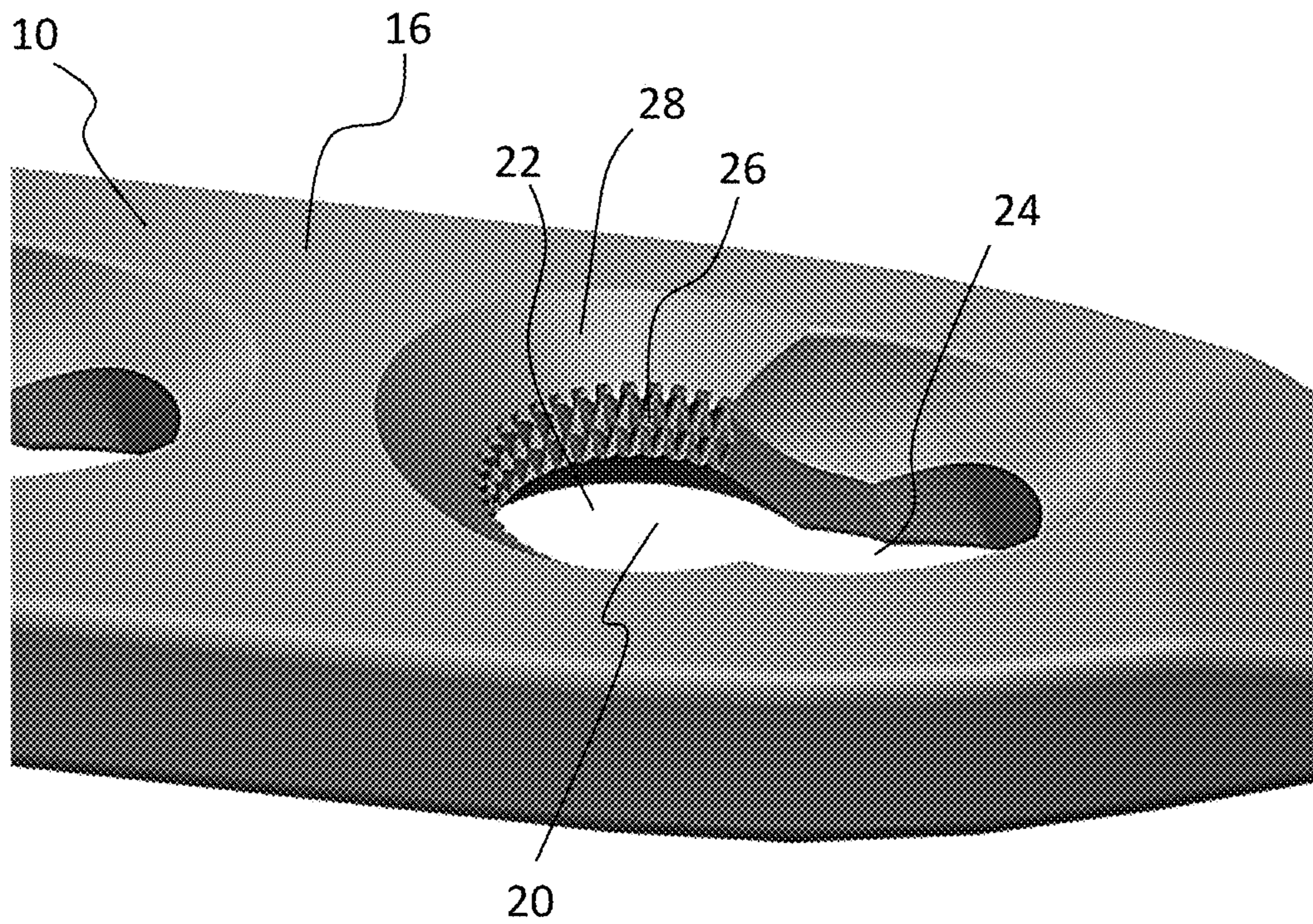


FIG. 3

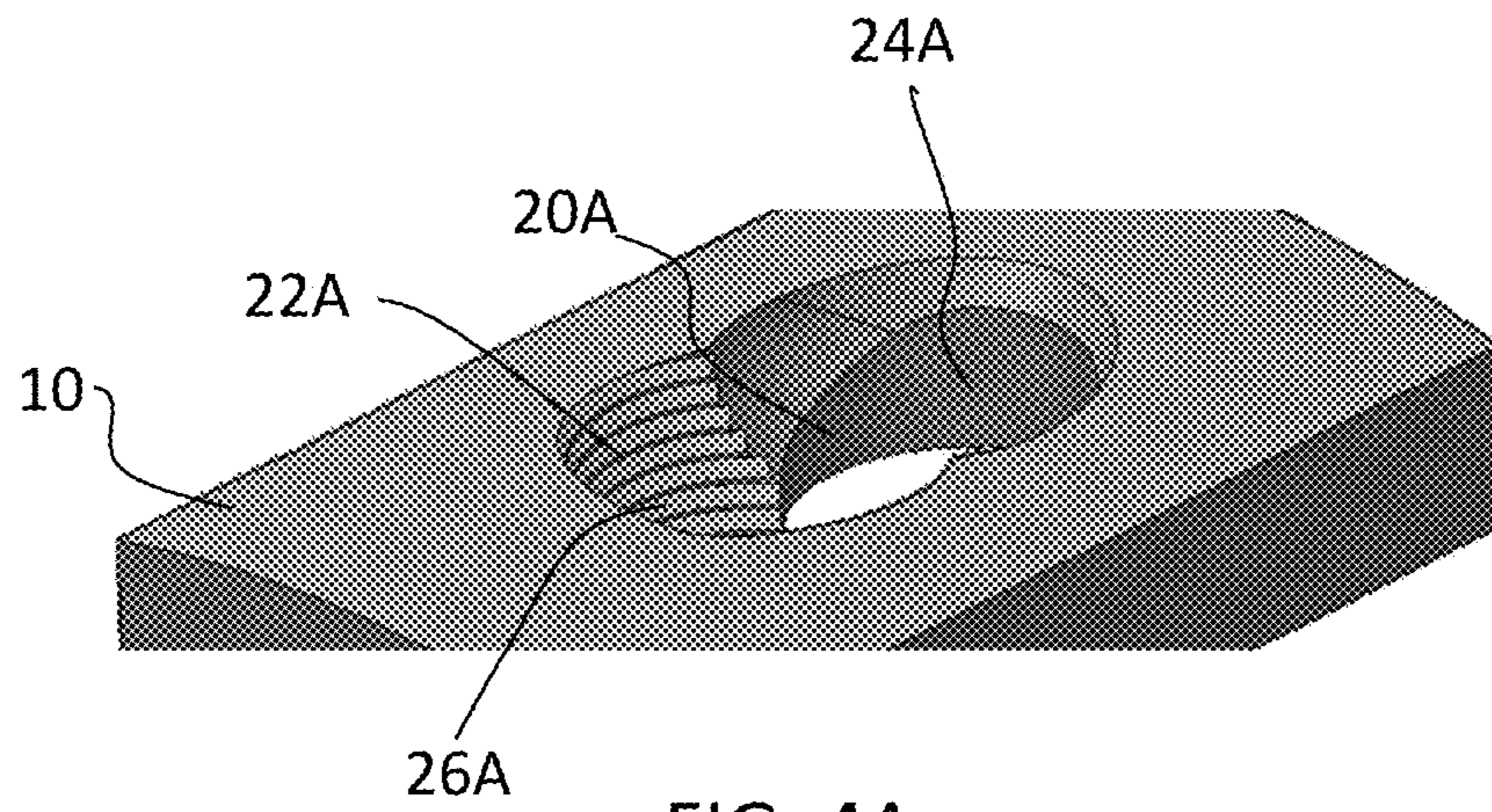


FIG. 4A

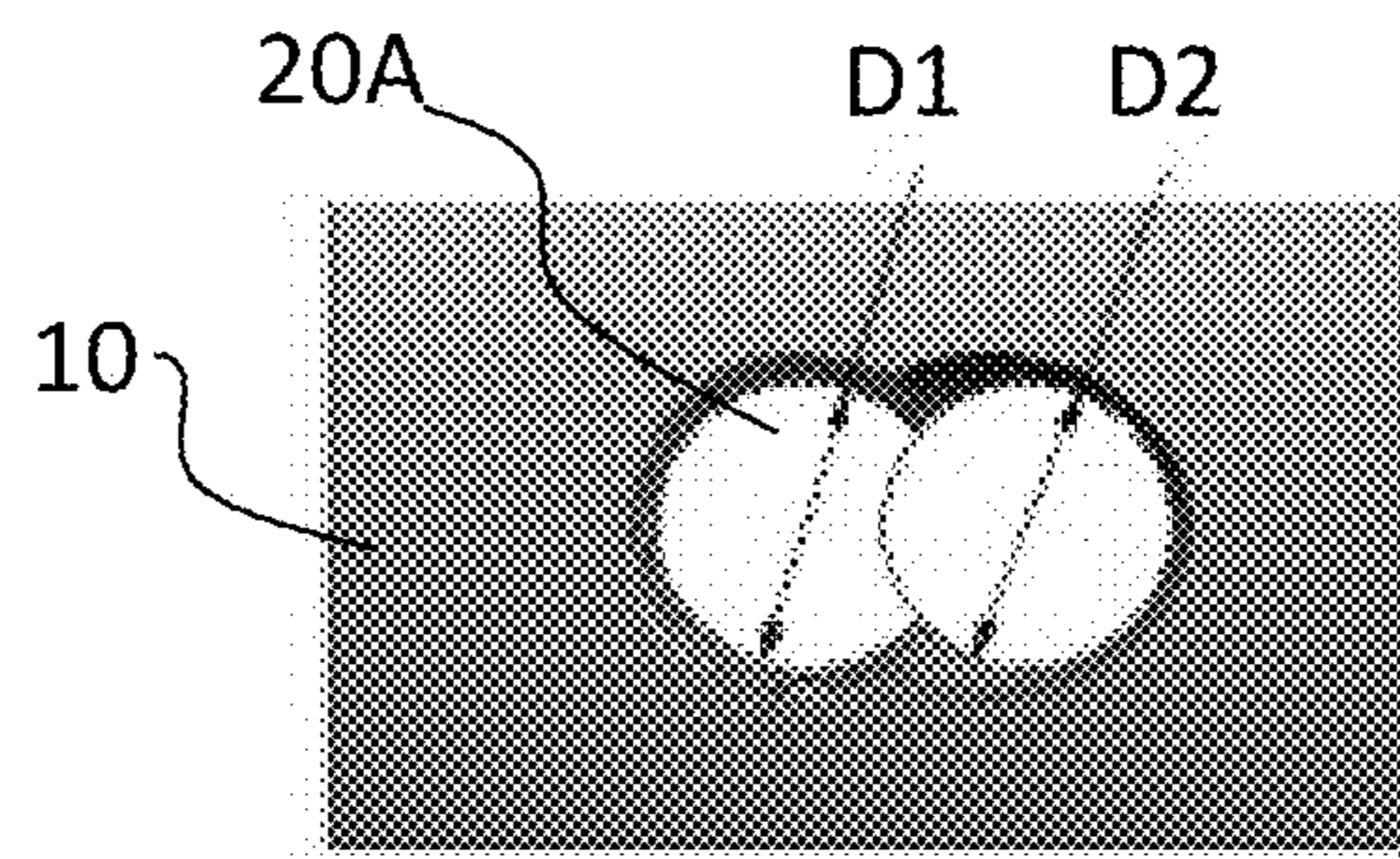


FIG. 4B

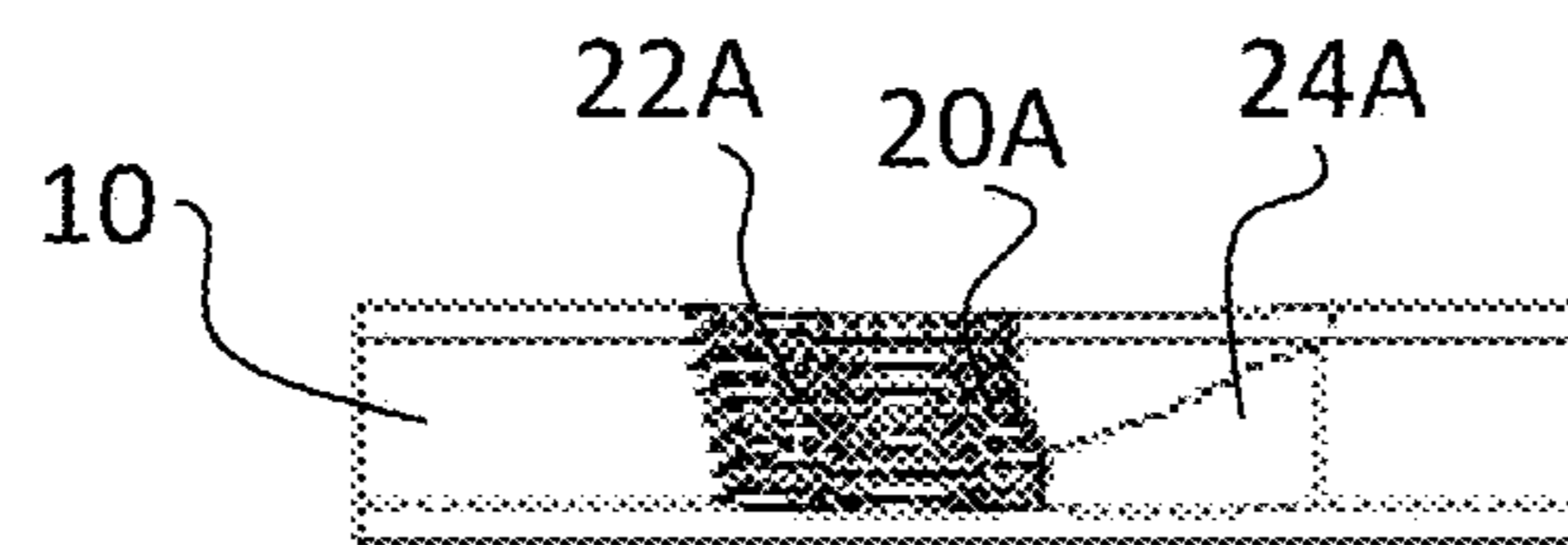


FIG. 4C

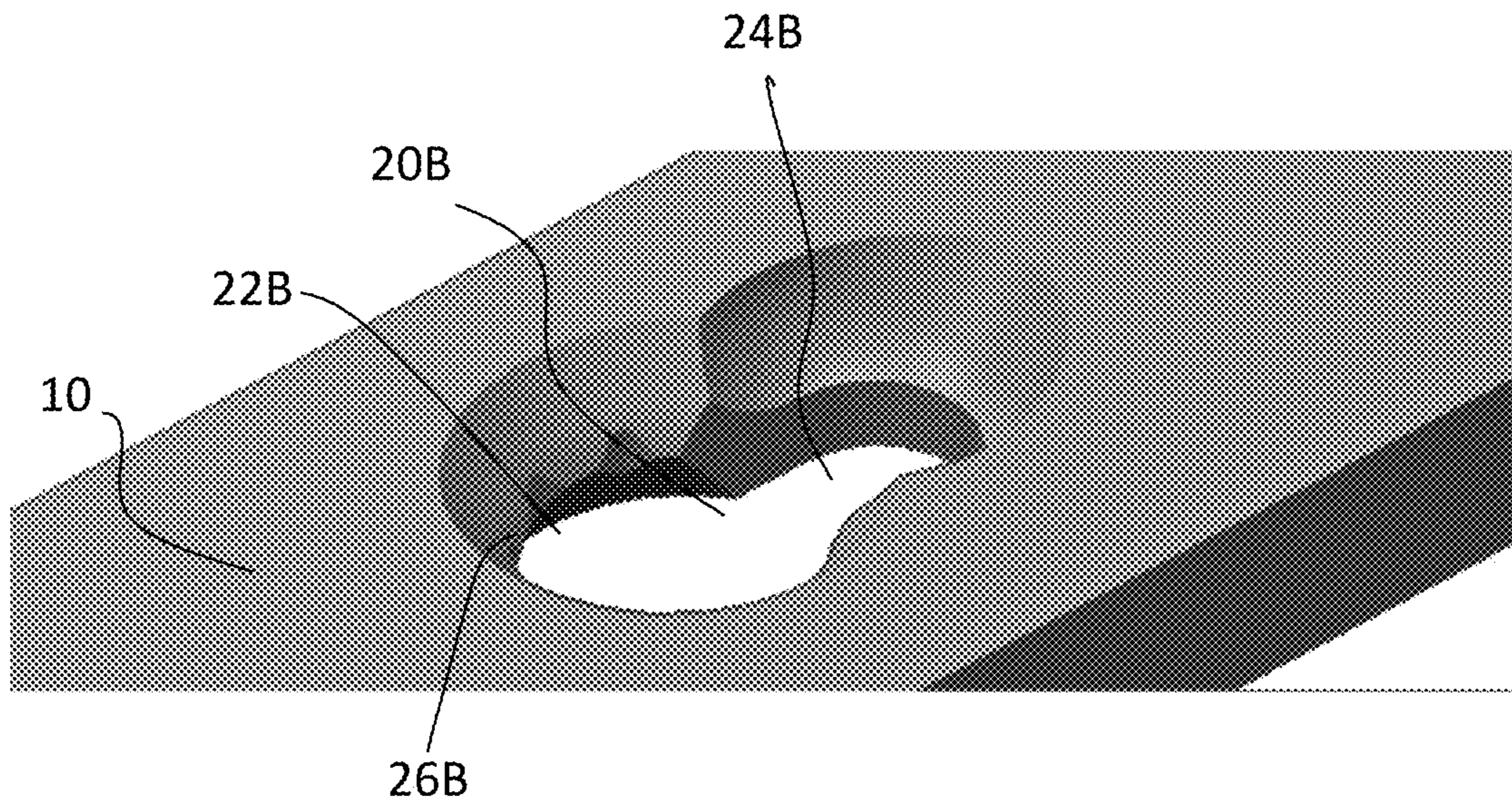


FIG. 5A

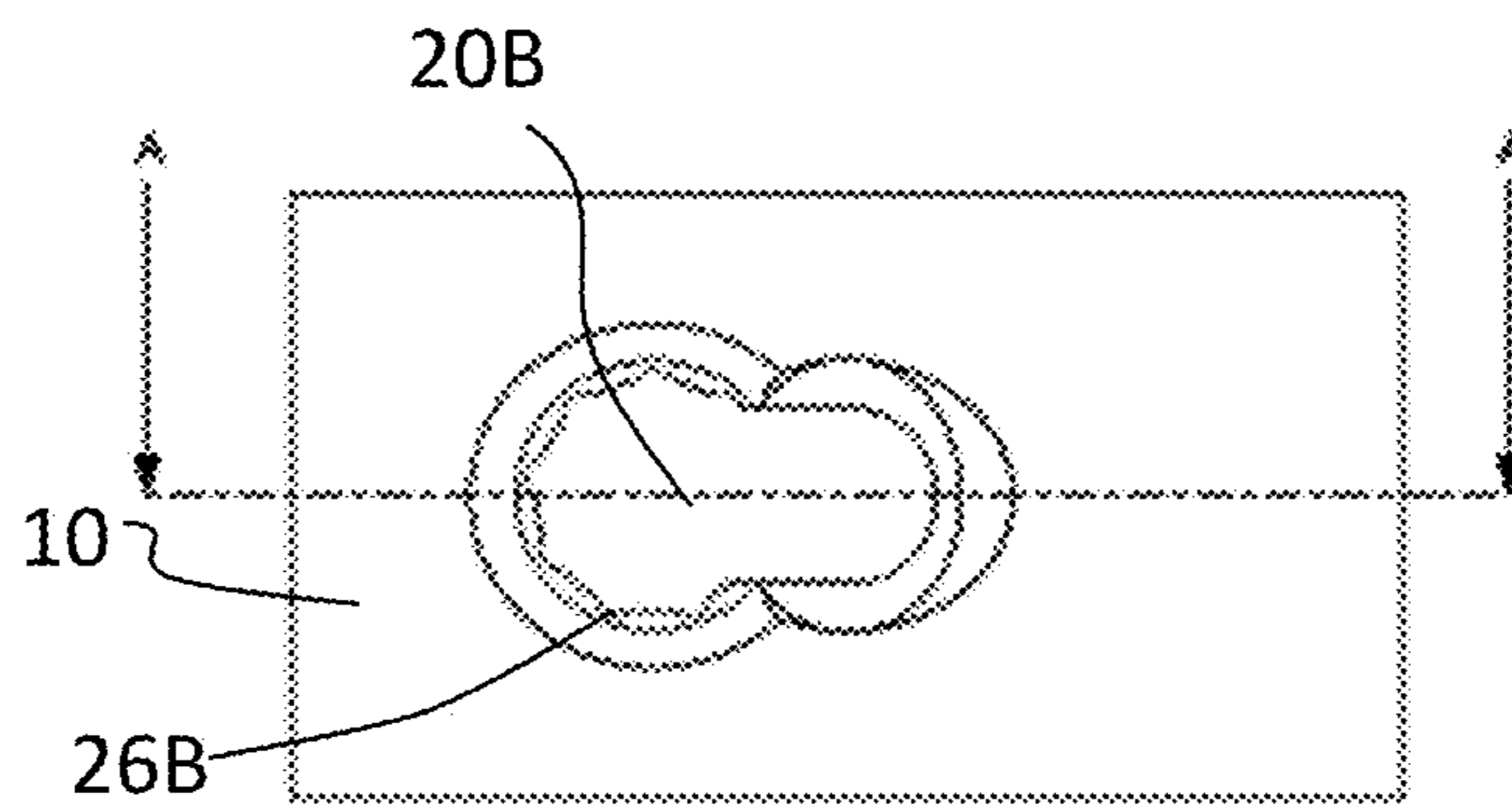


FIG. 5B

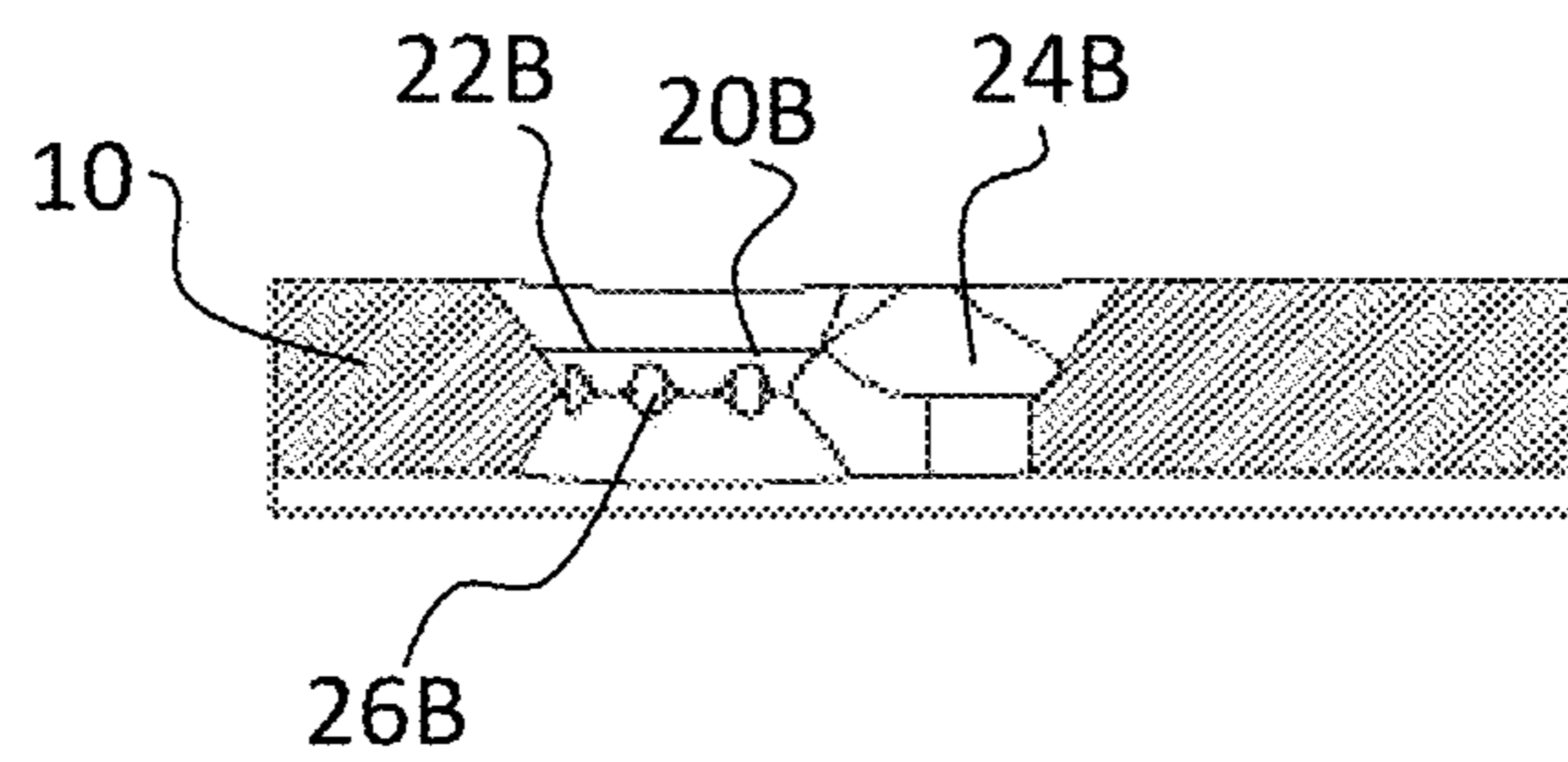


FIG. 5C

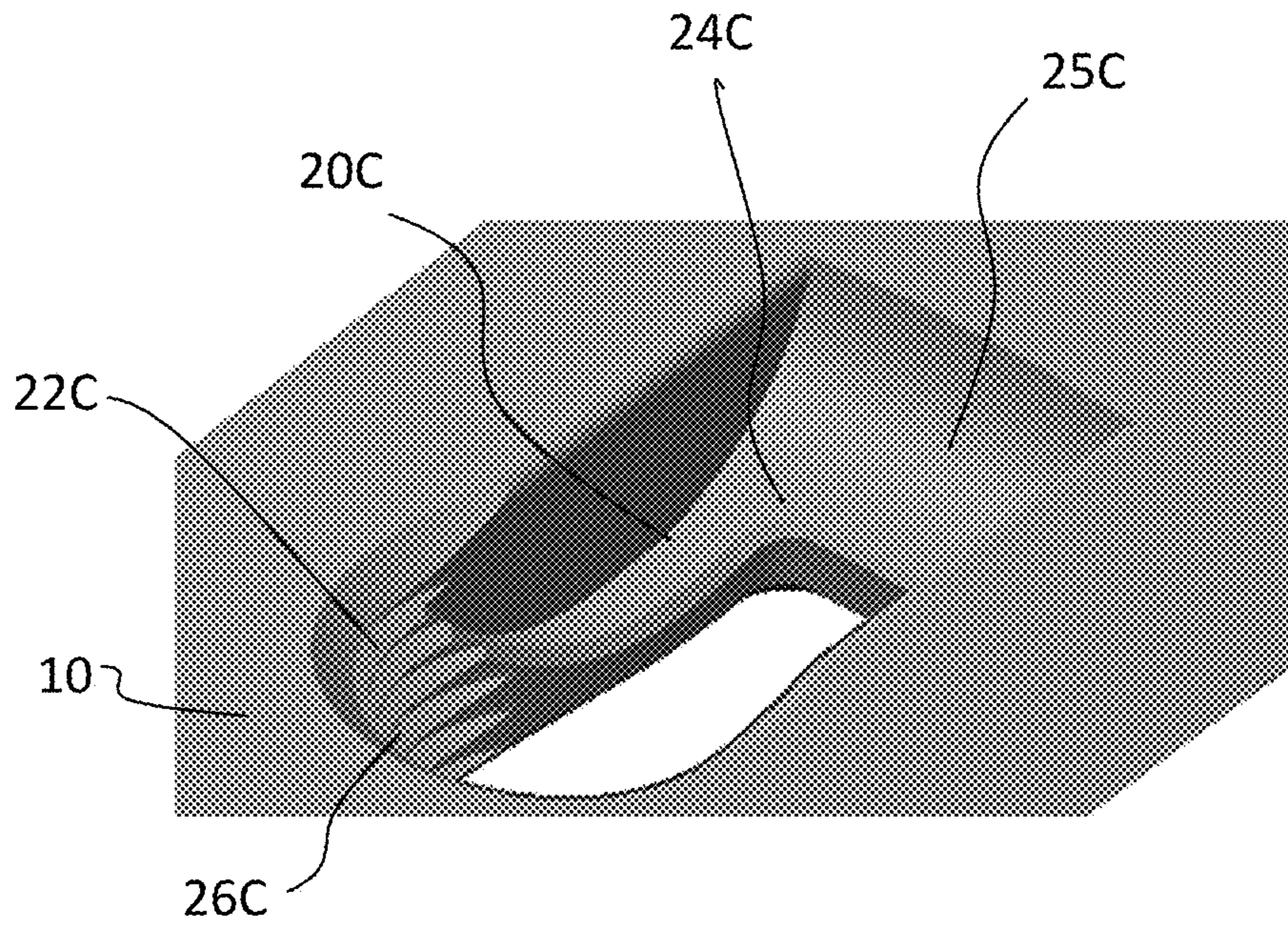


FIG. 6A

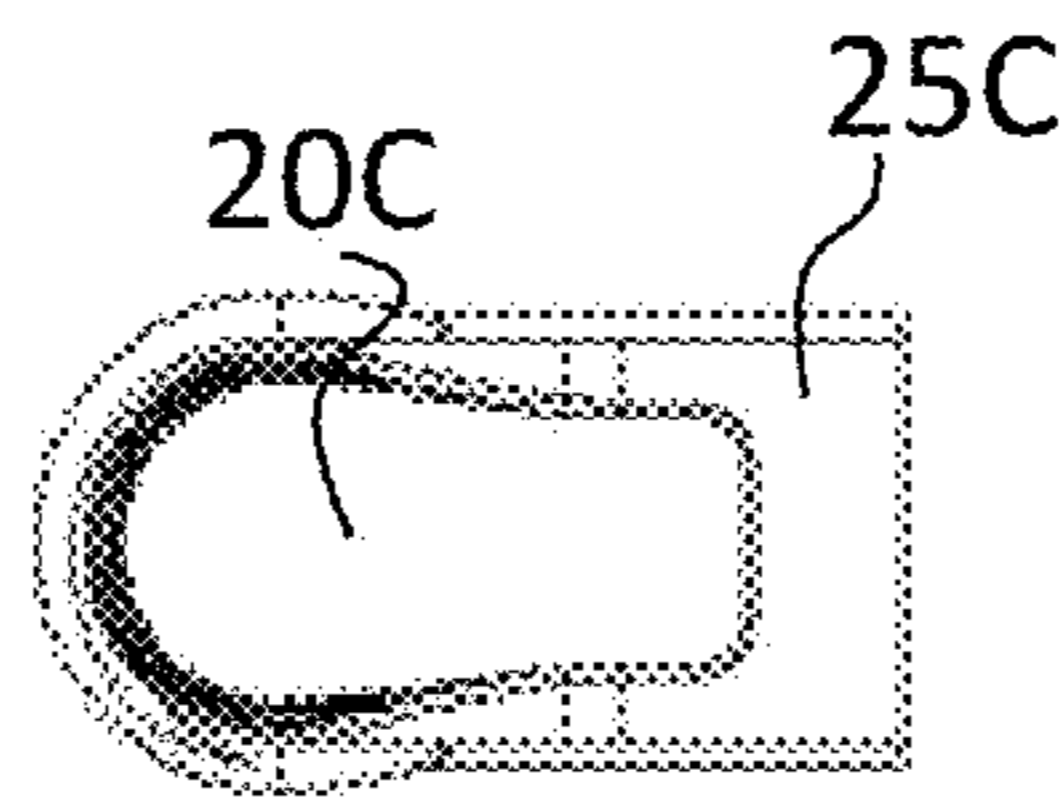


FIG. 6B

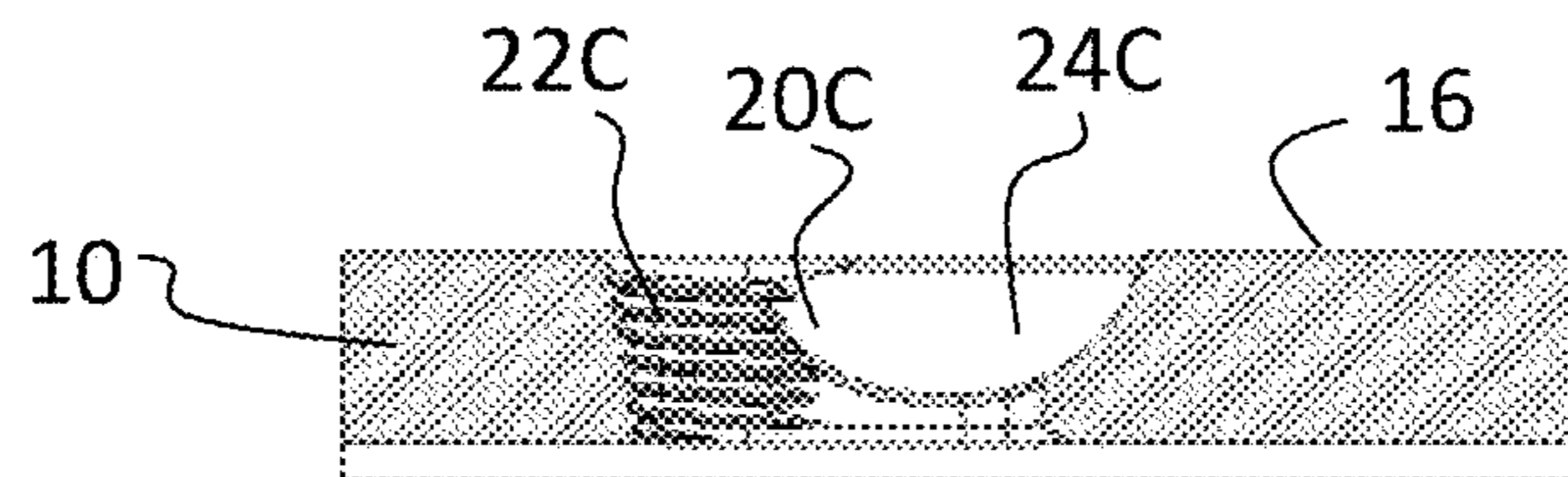


FIG. 6C

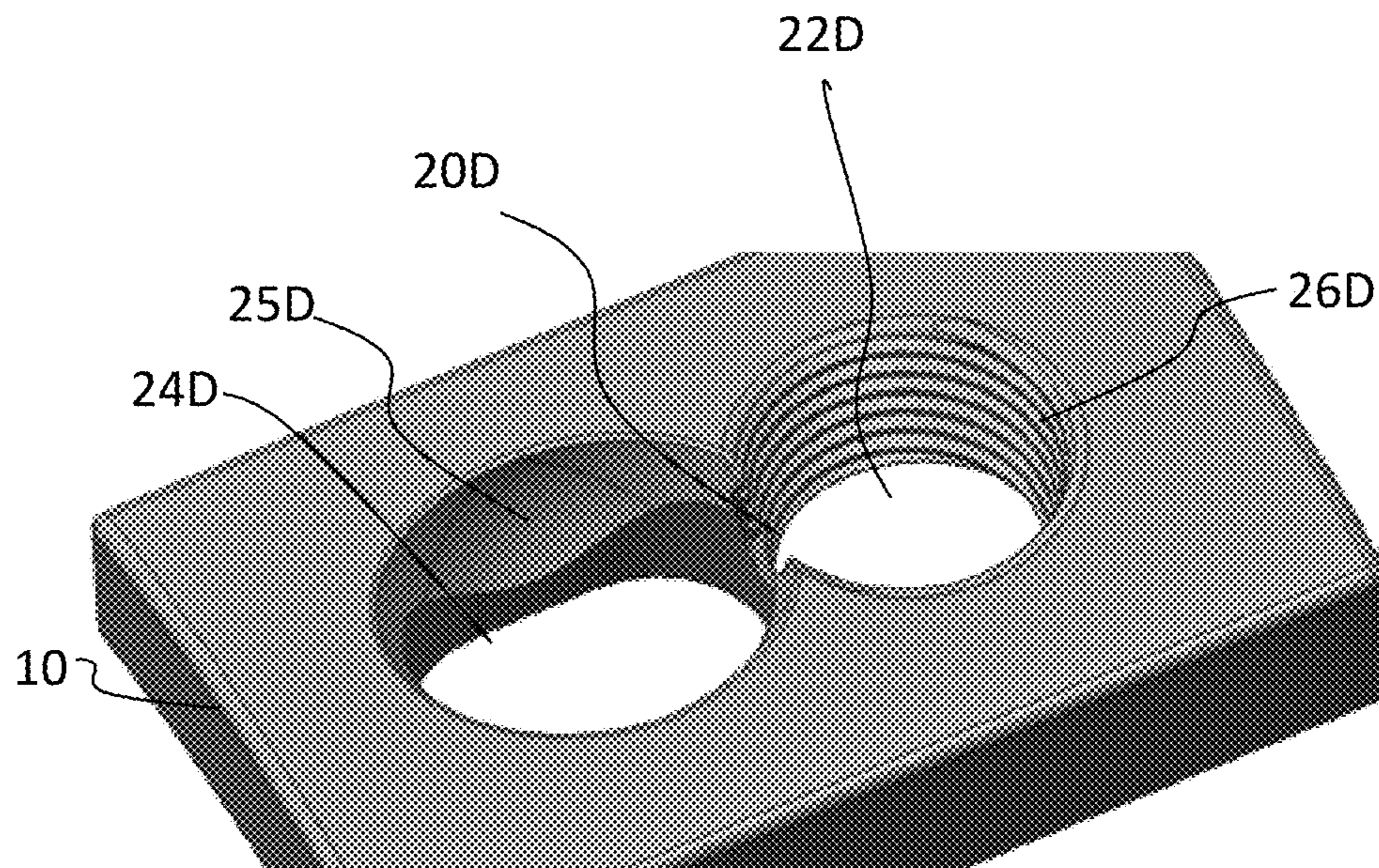


FIG. 7A

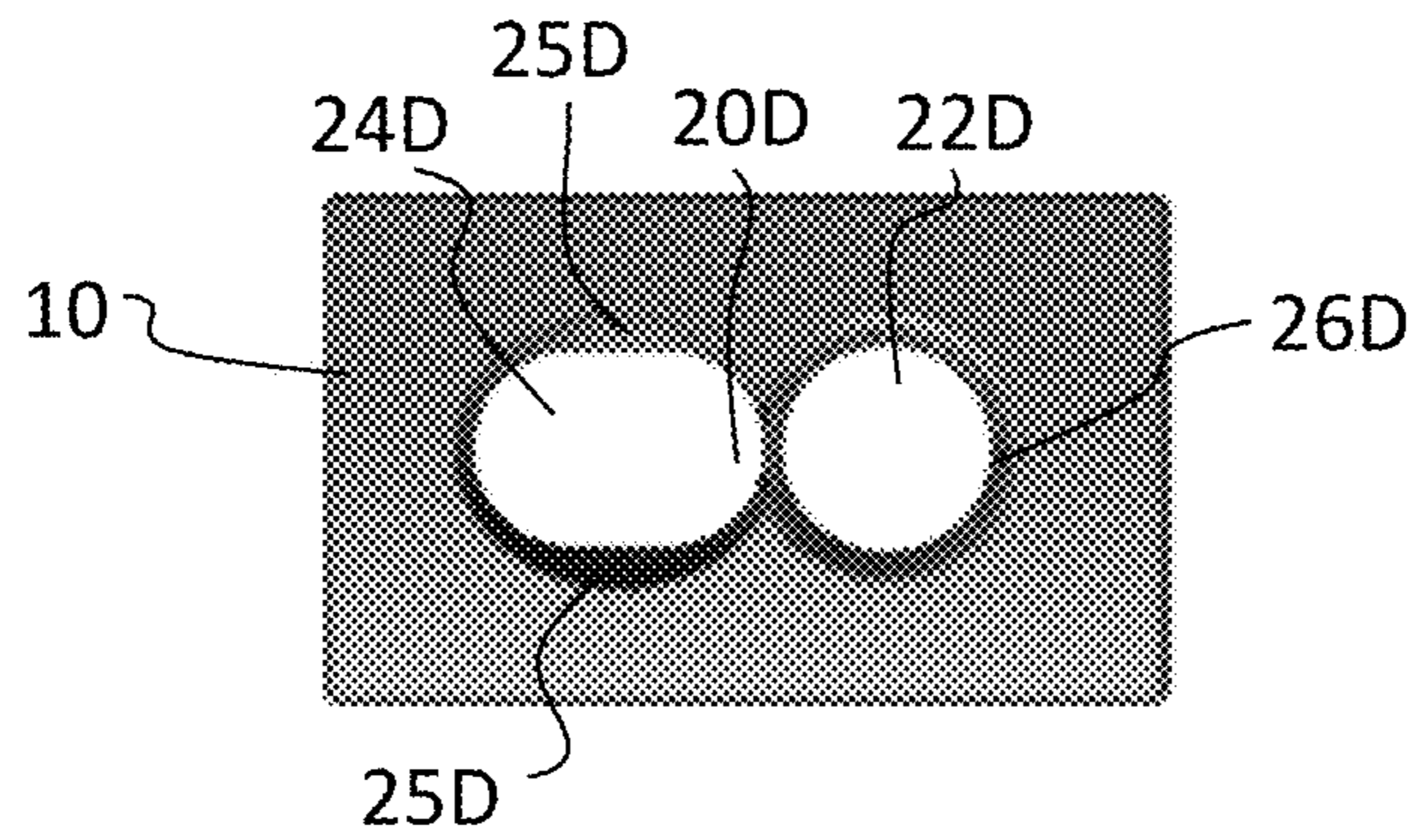


FIG. 7B

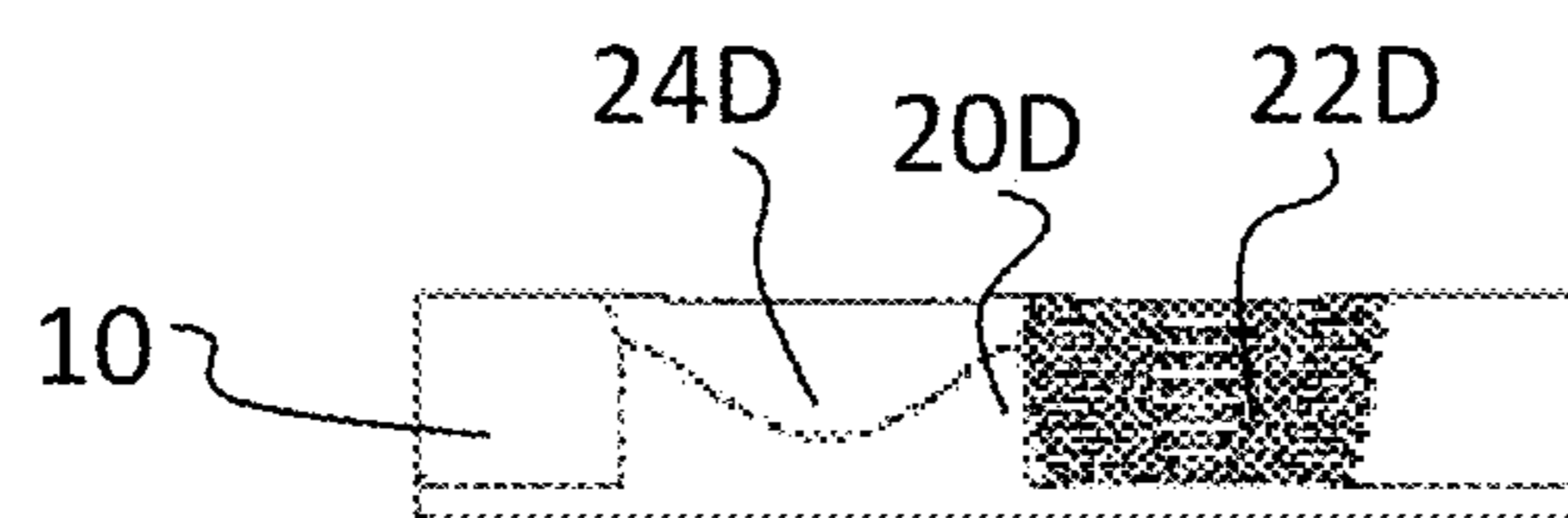


FIG. 7C

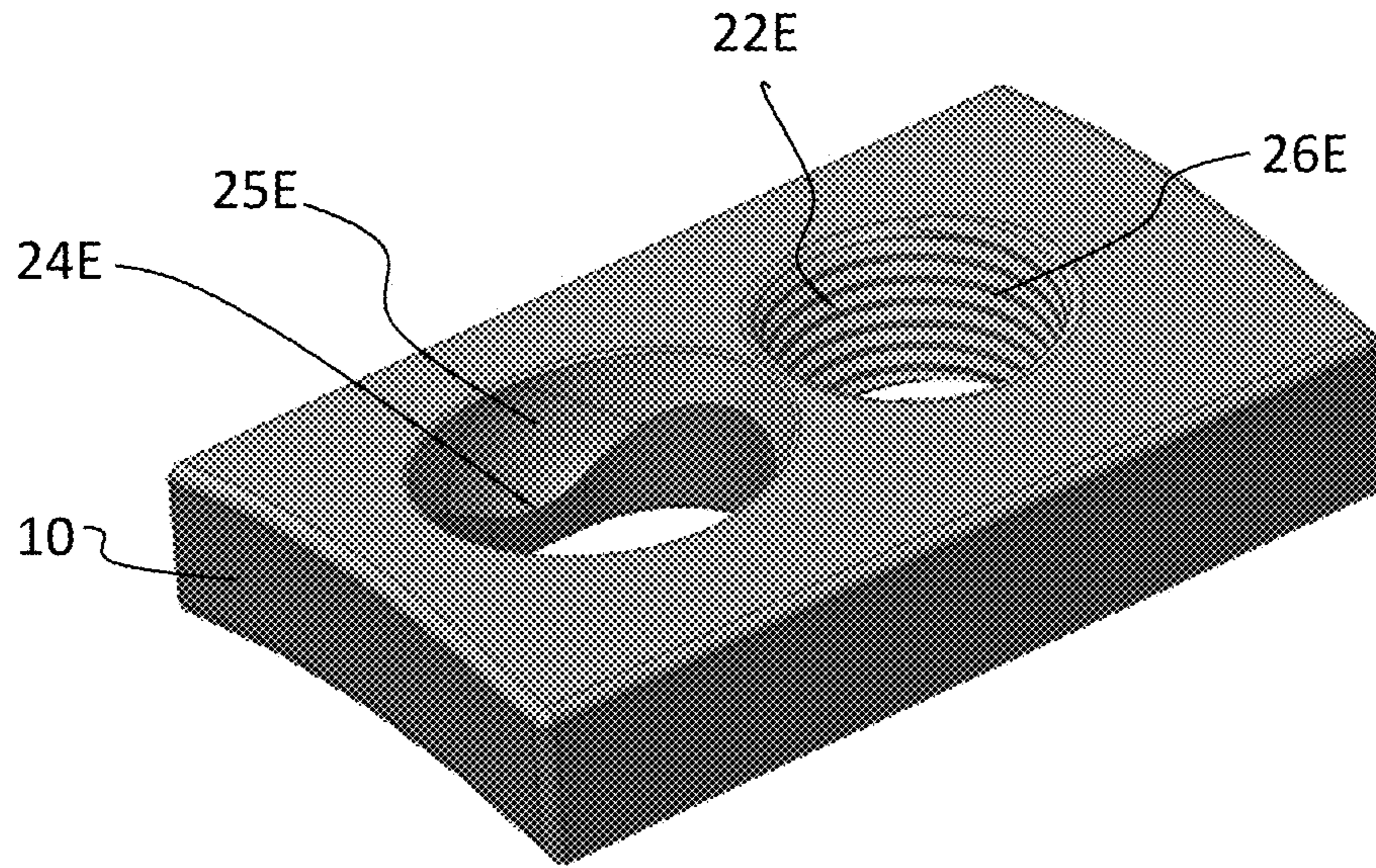


FIG. 8A

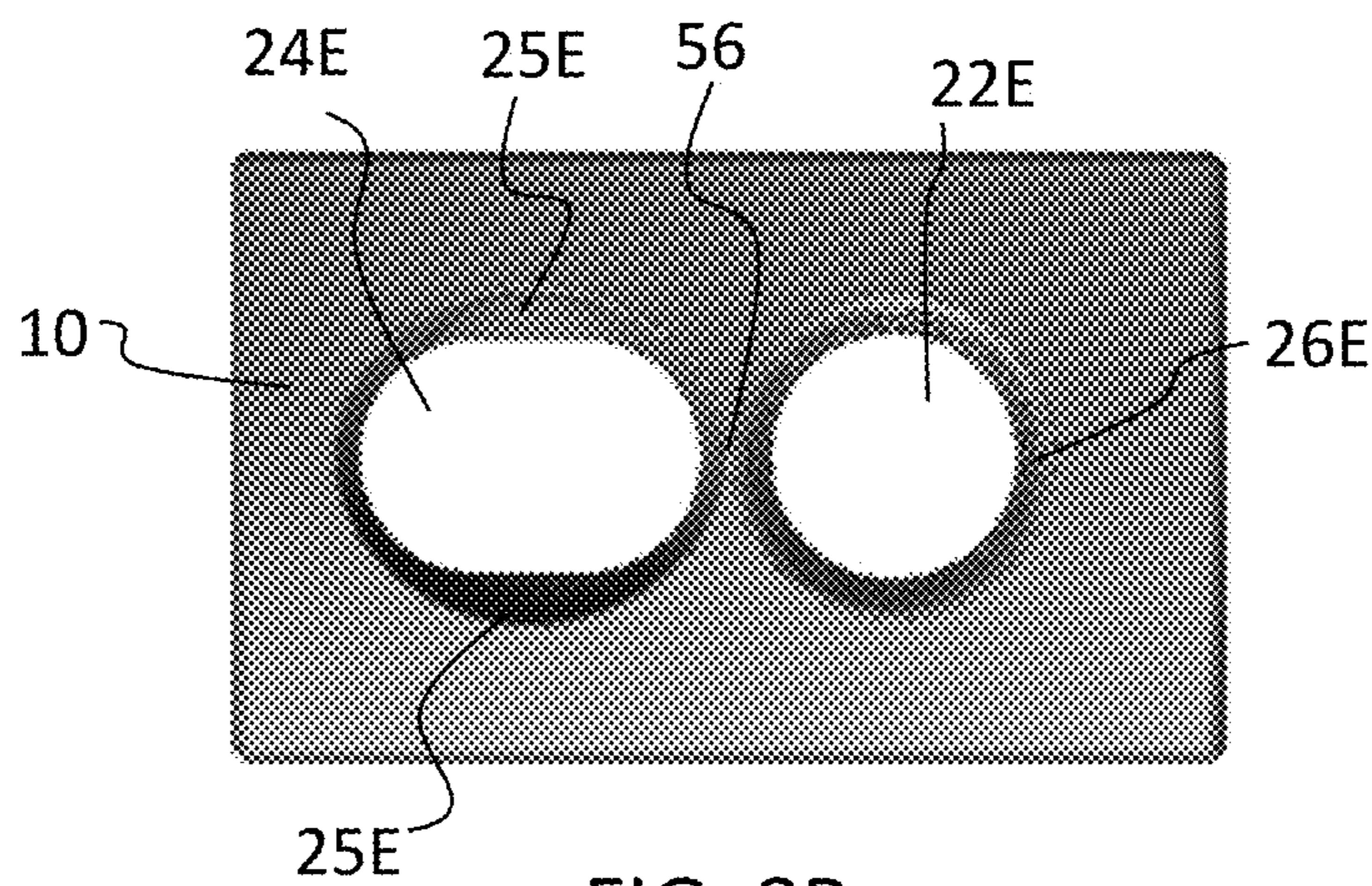


FIG. 8B

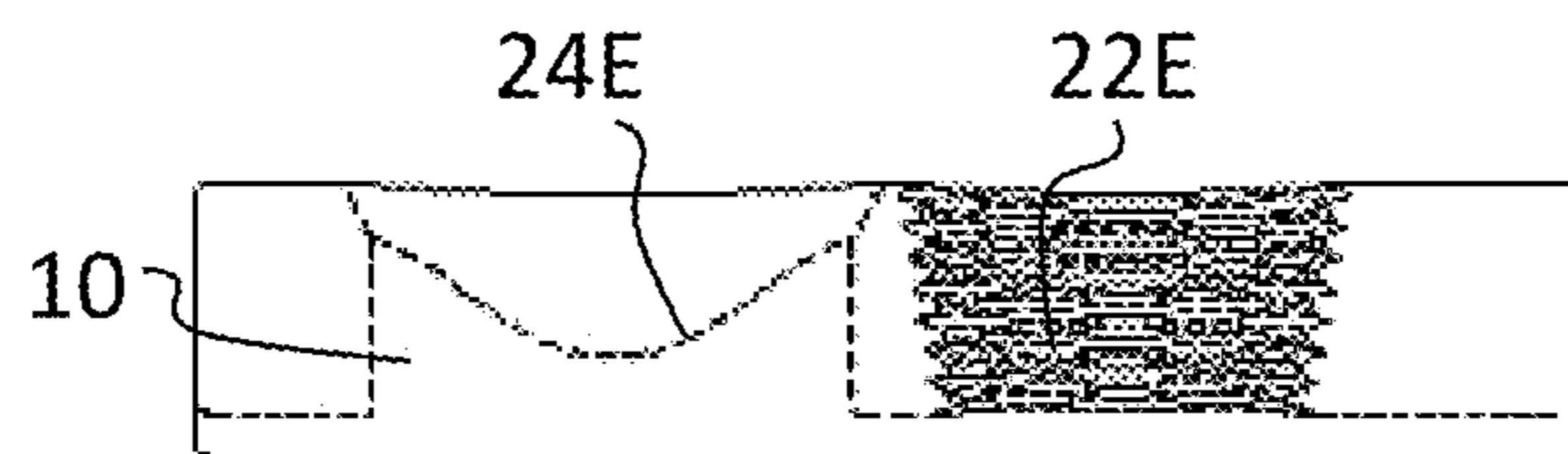


FIG. 8C

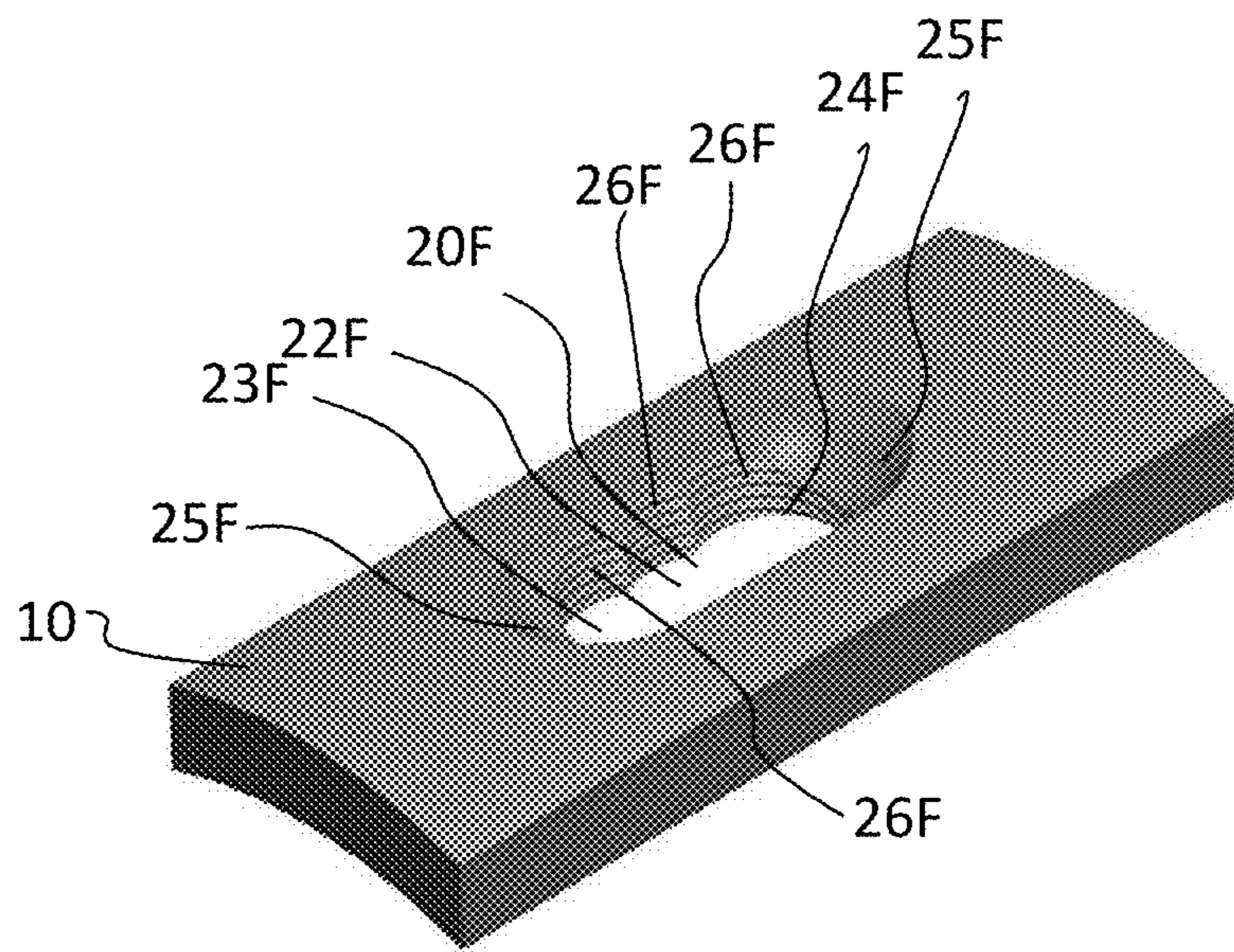


FIG. 9A

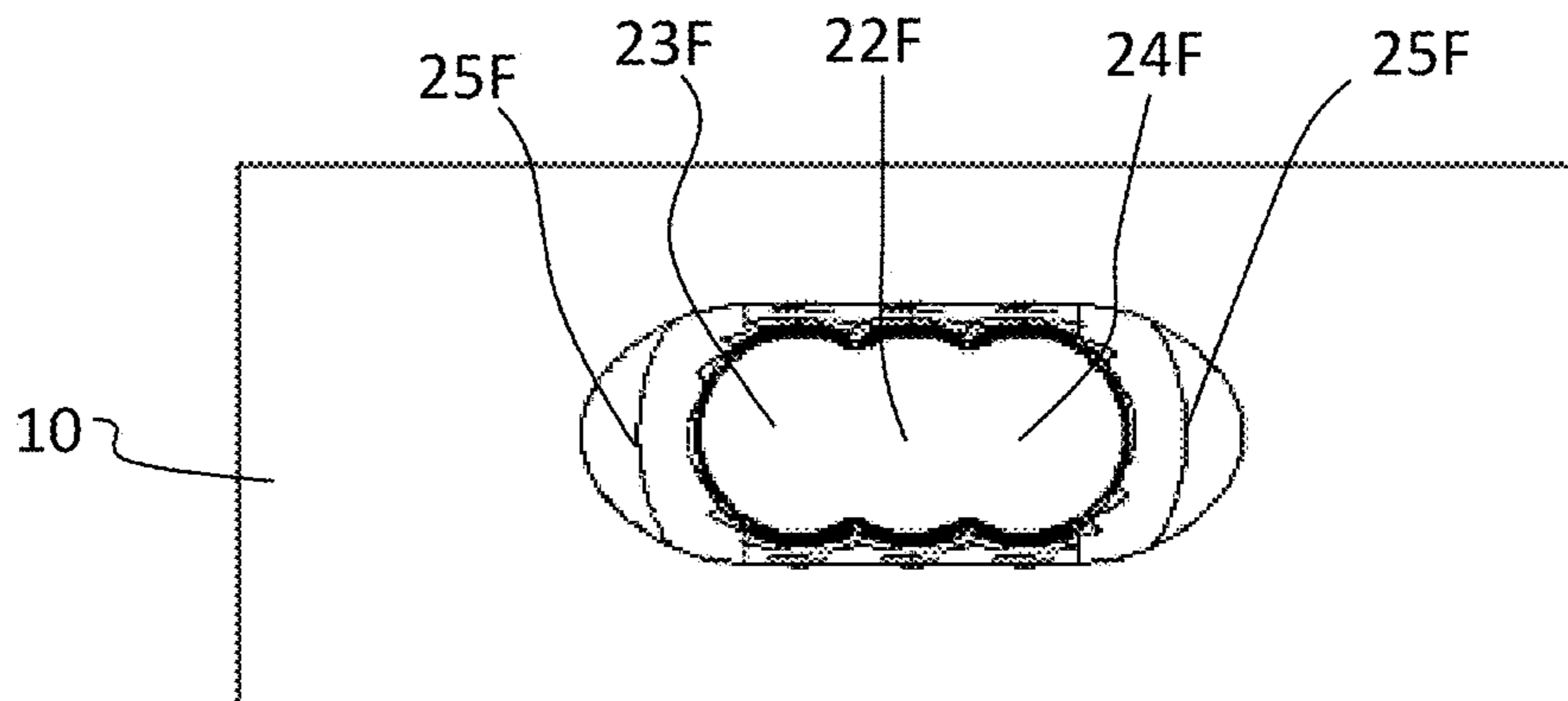


FIG. 9B

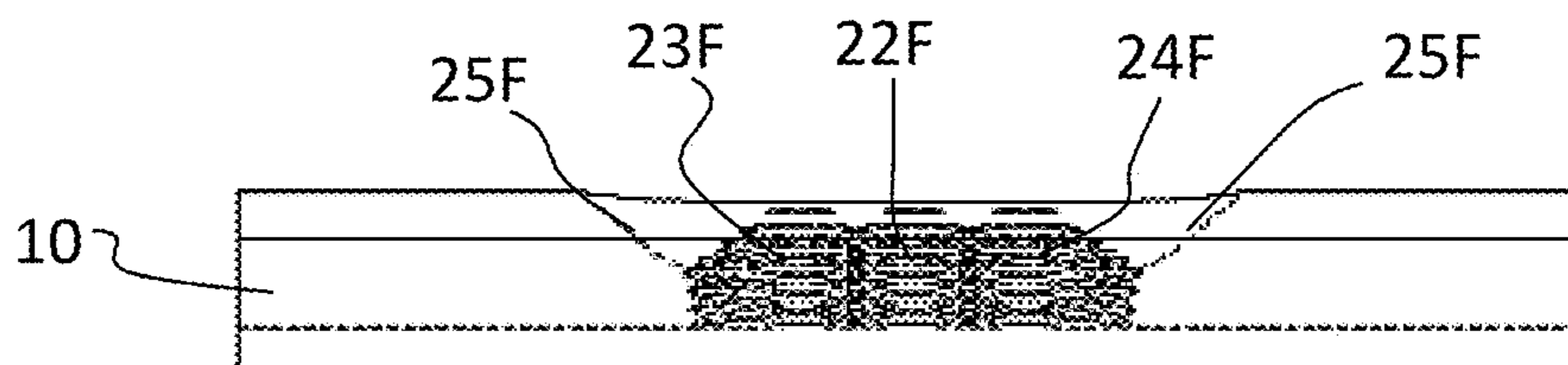


FIG. 9C

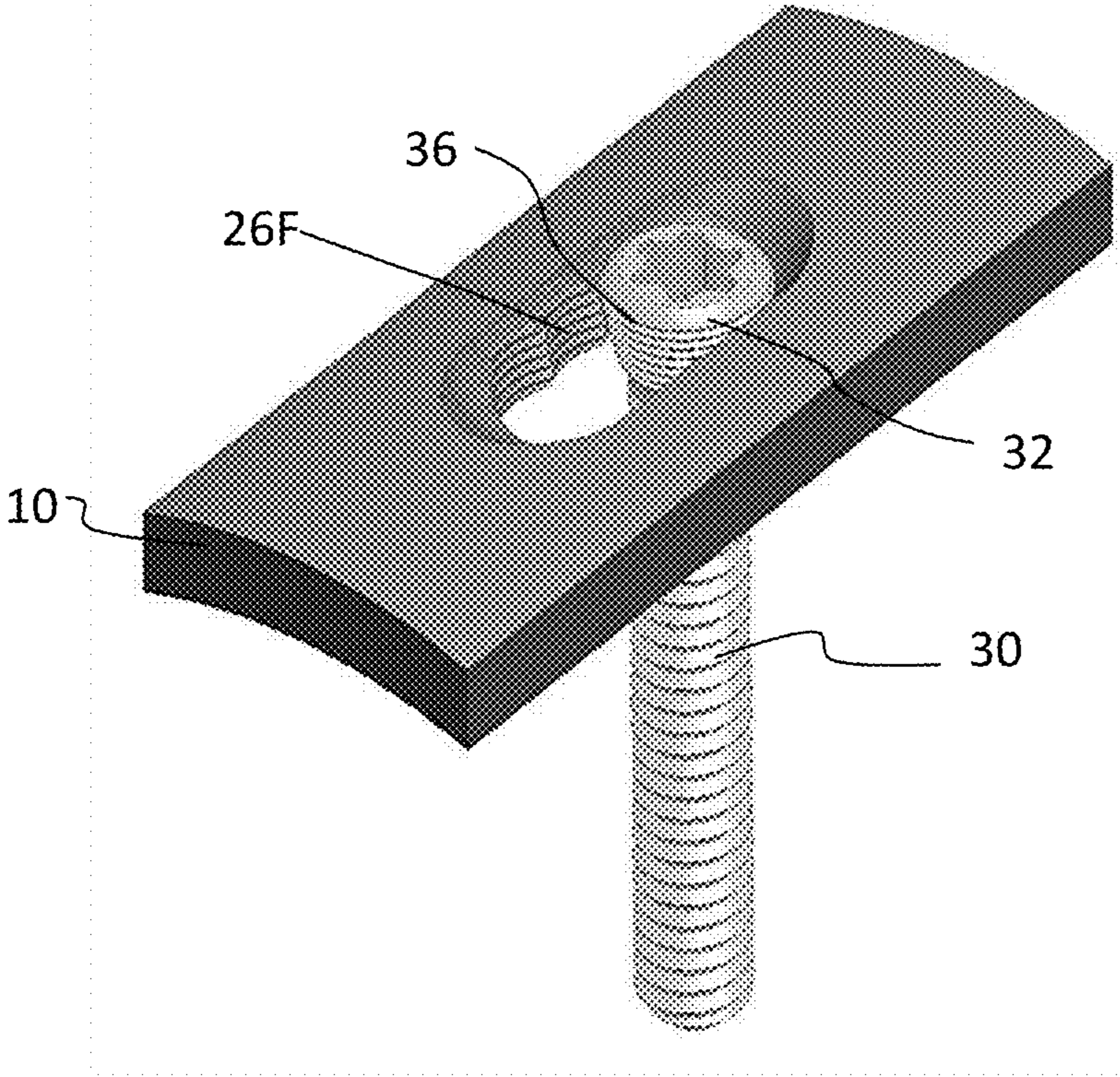


FIG. 9D

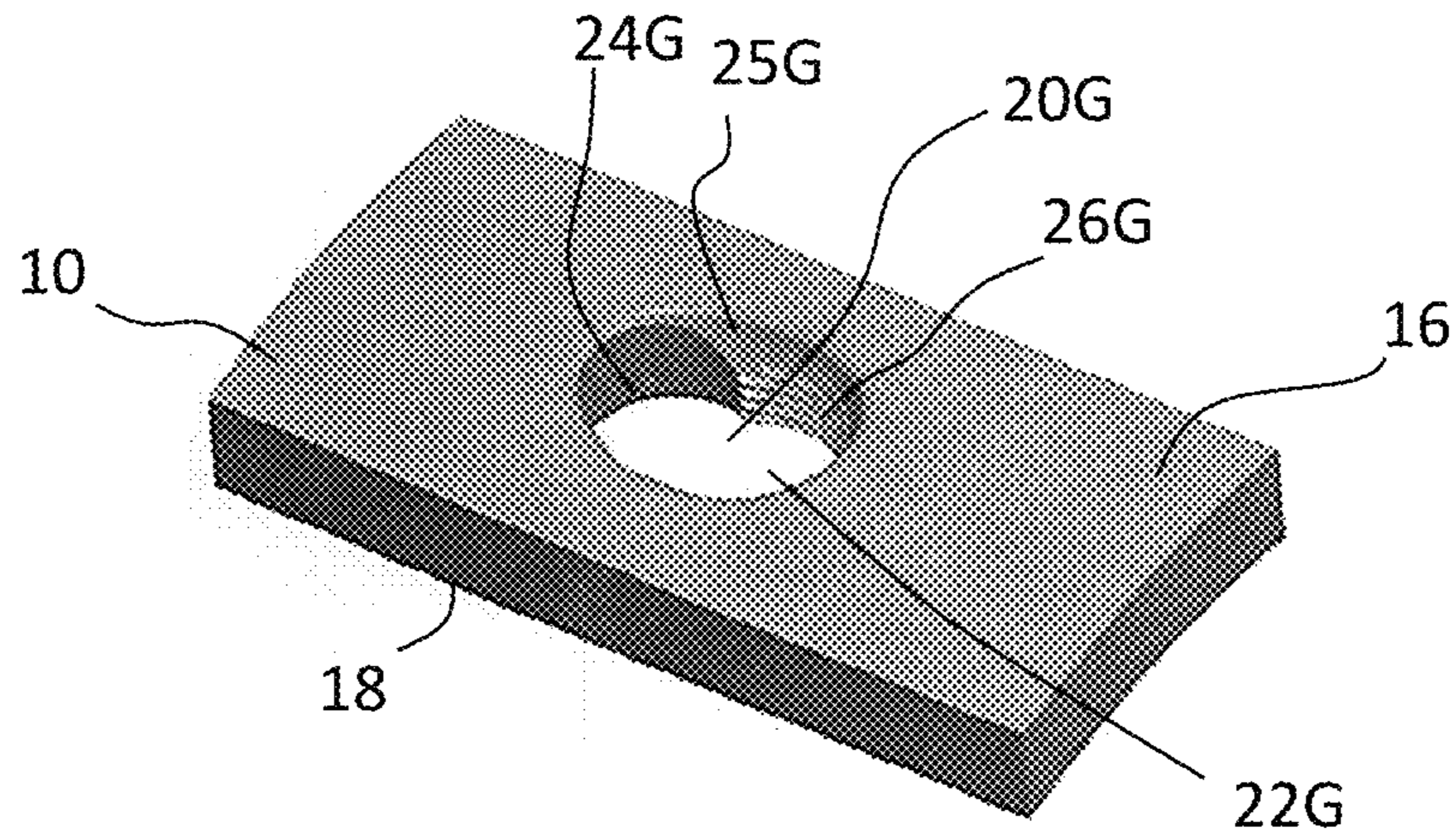


FIG. 10A

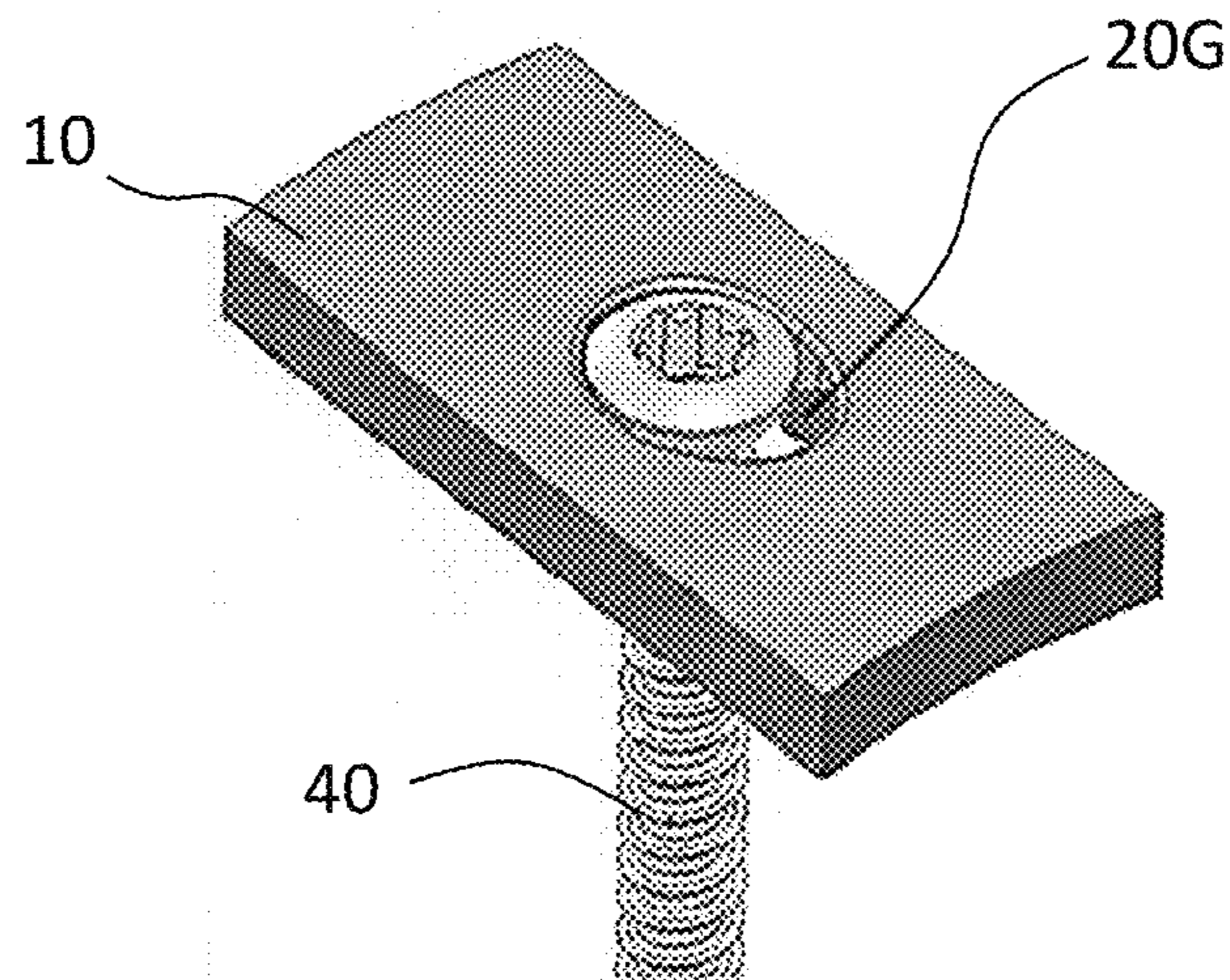


FIG. 10B

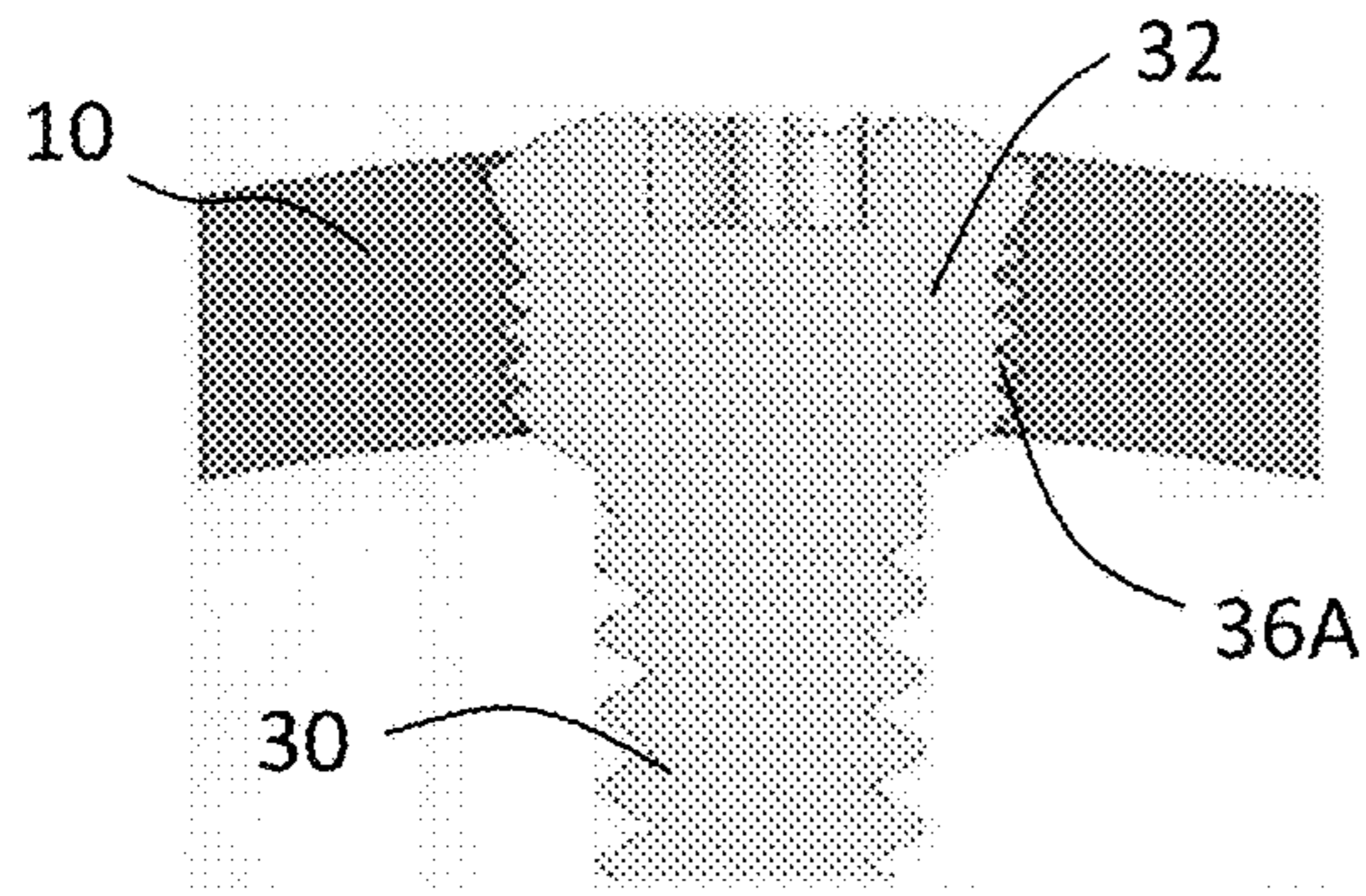


FIG. 11A

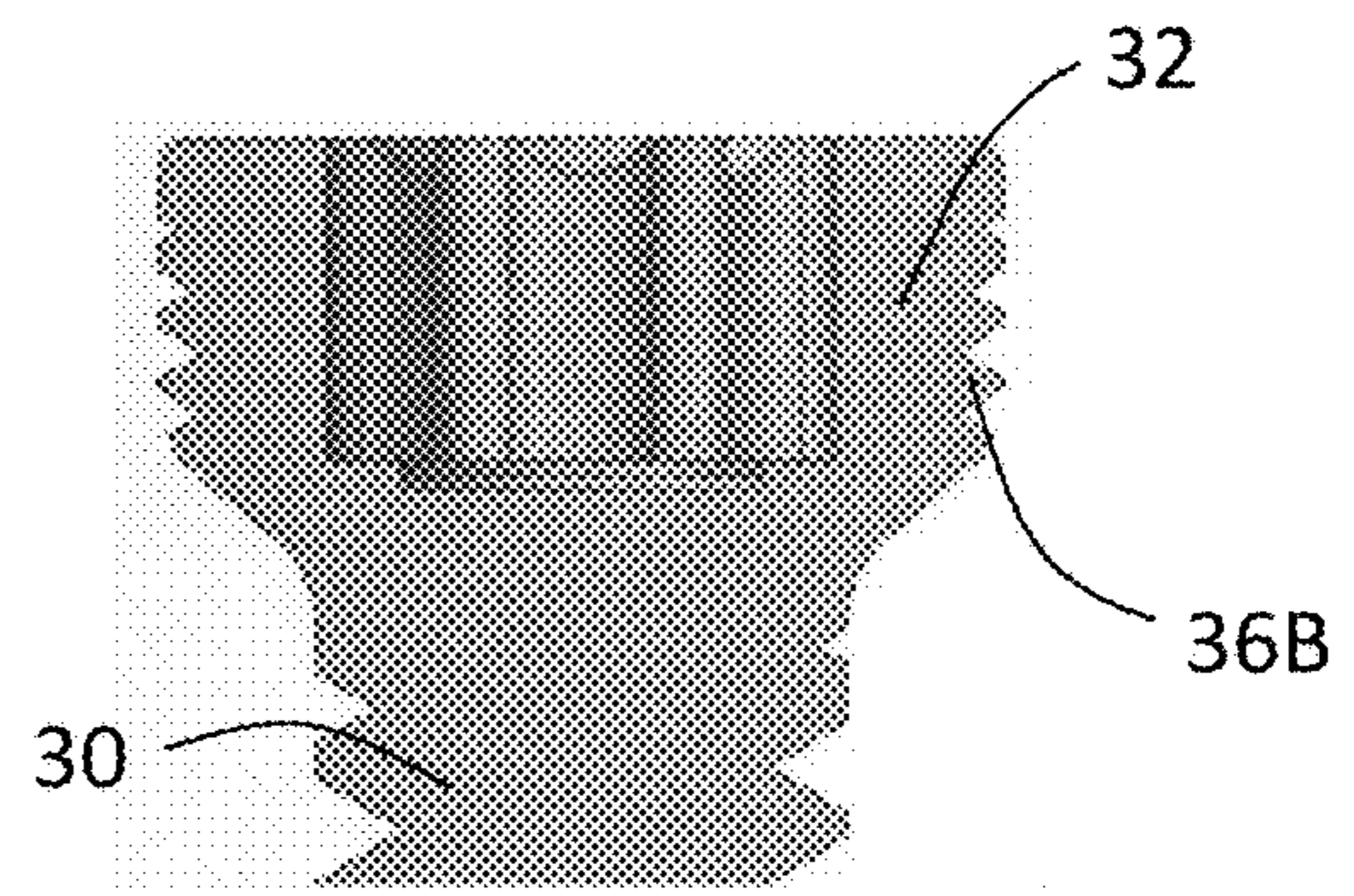


FIG. 11B

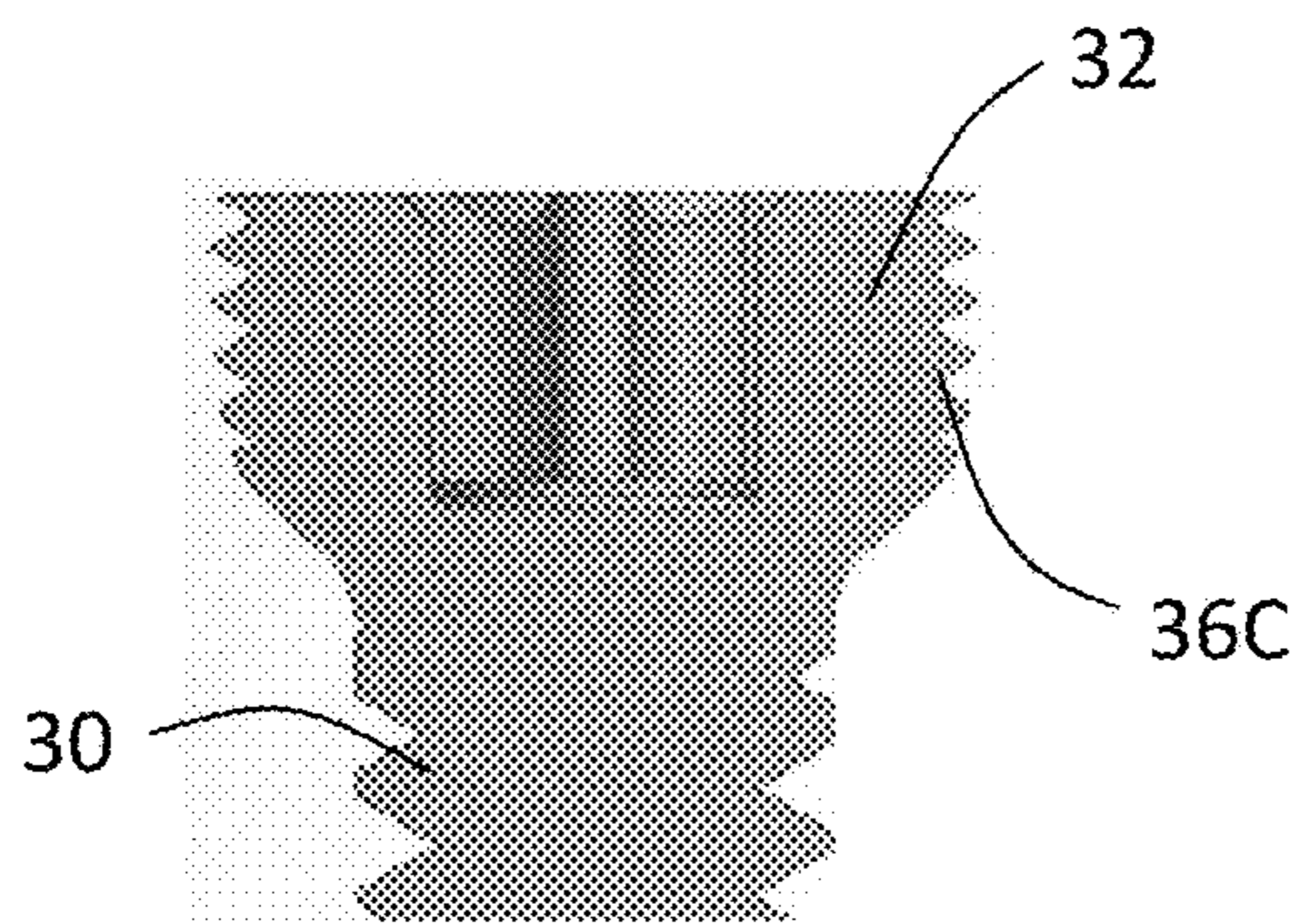


FIG. 11C

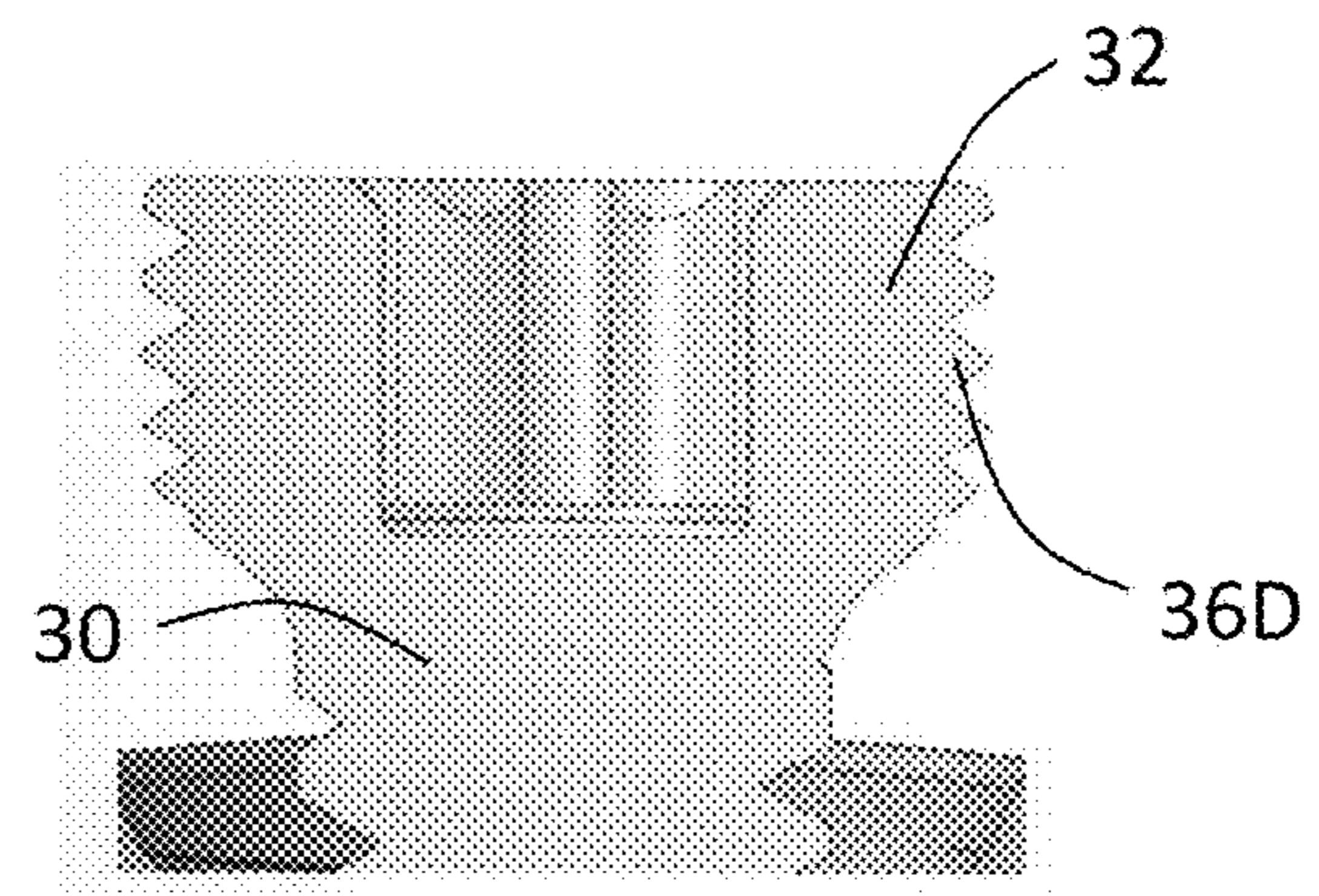


FIG. 11D

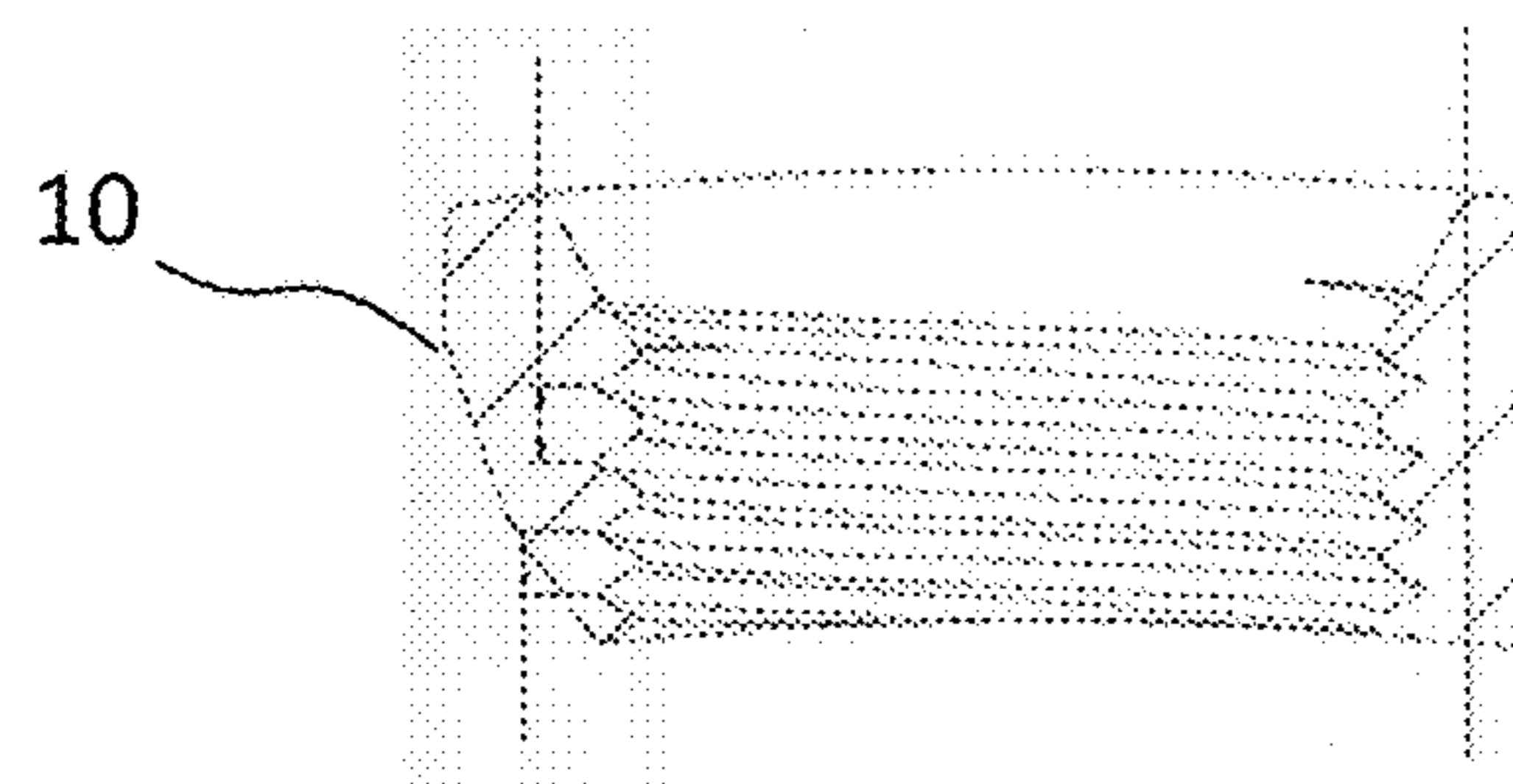


FIG. 11E

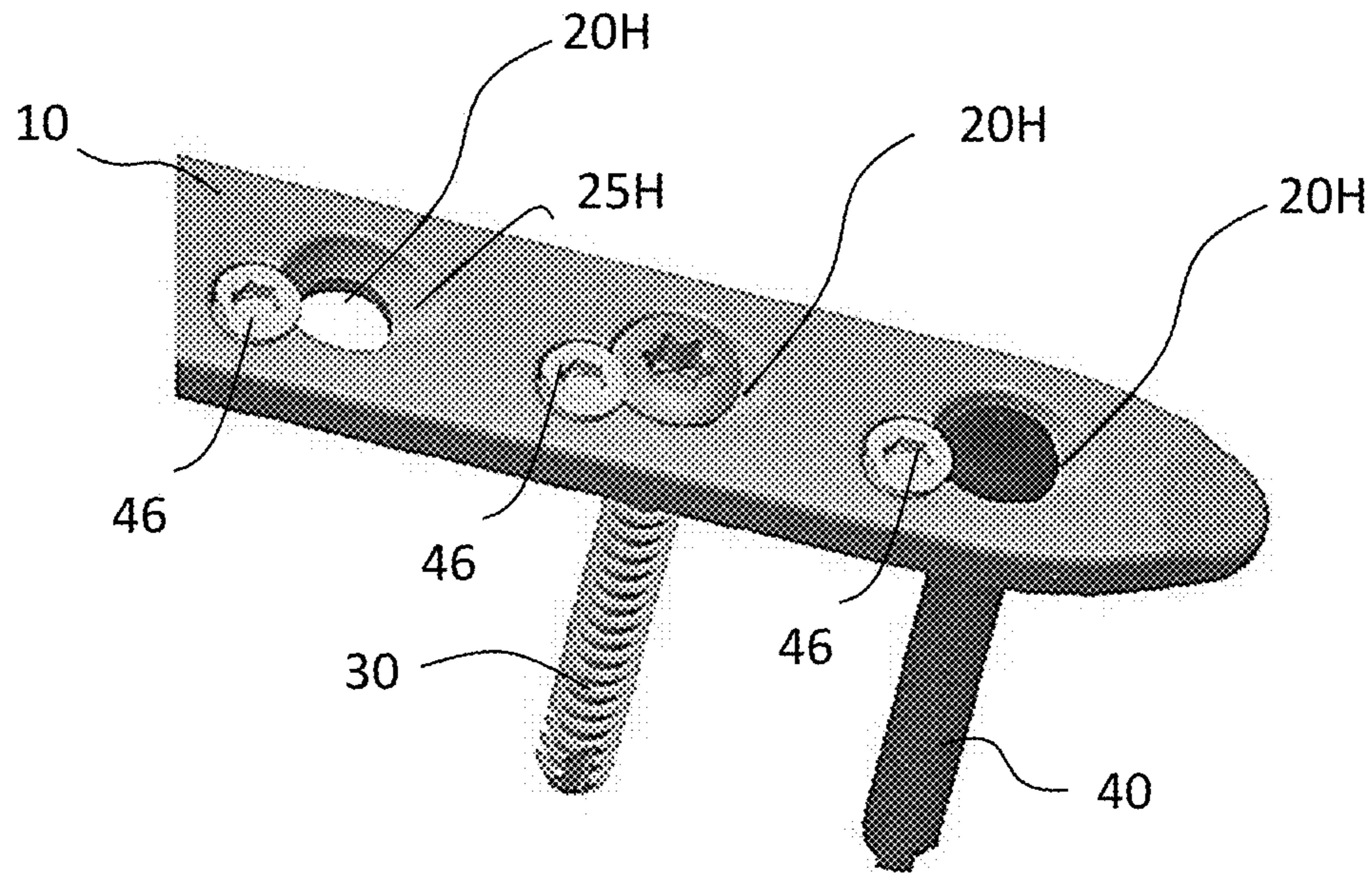


FIG. 12A

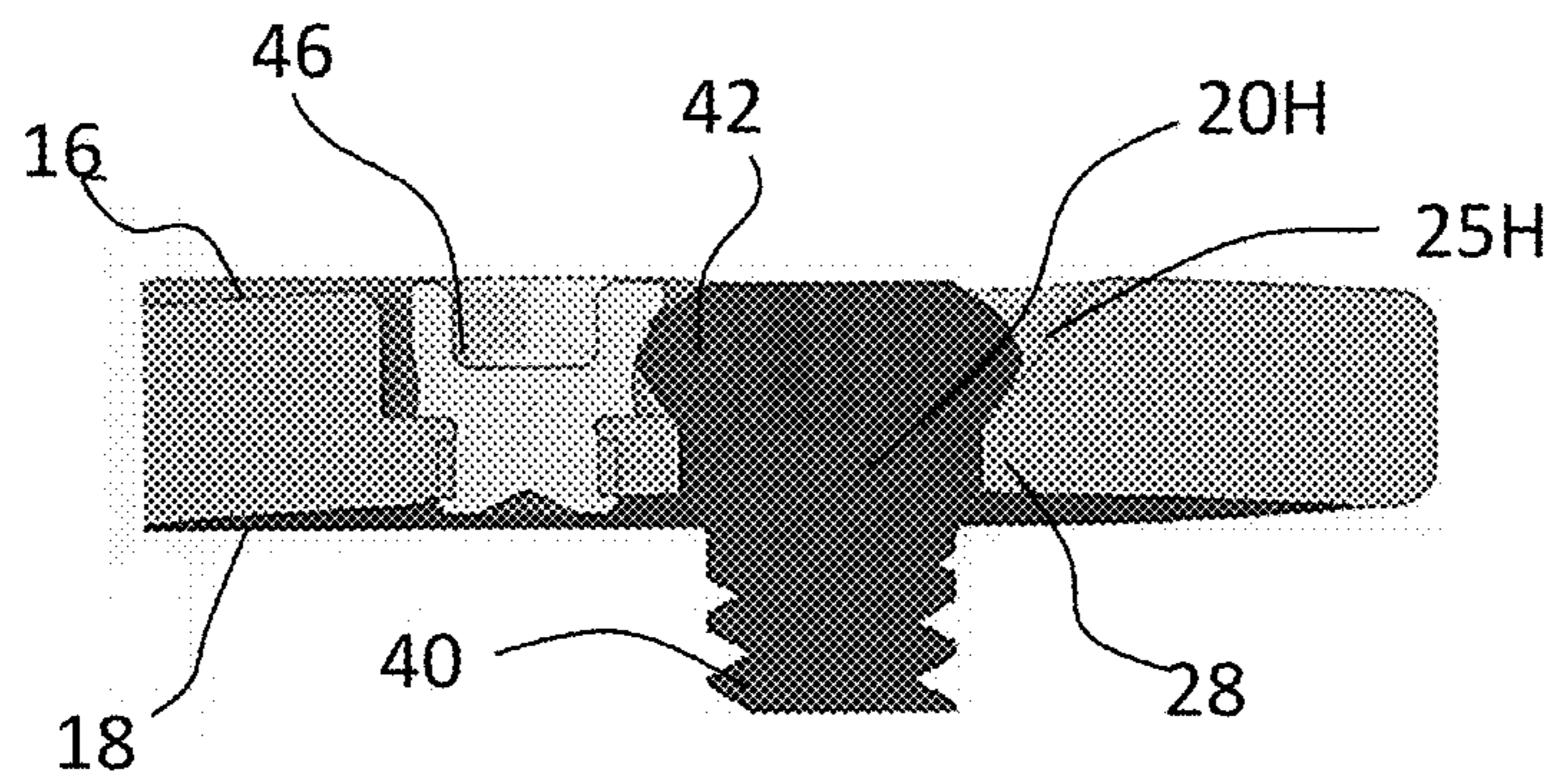


FIG. 12B

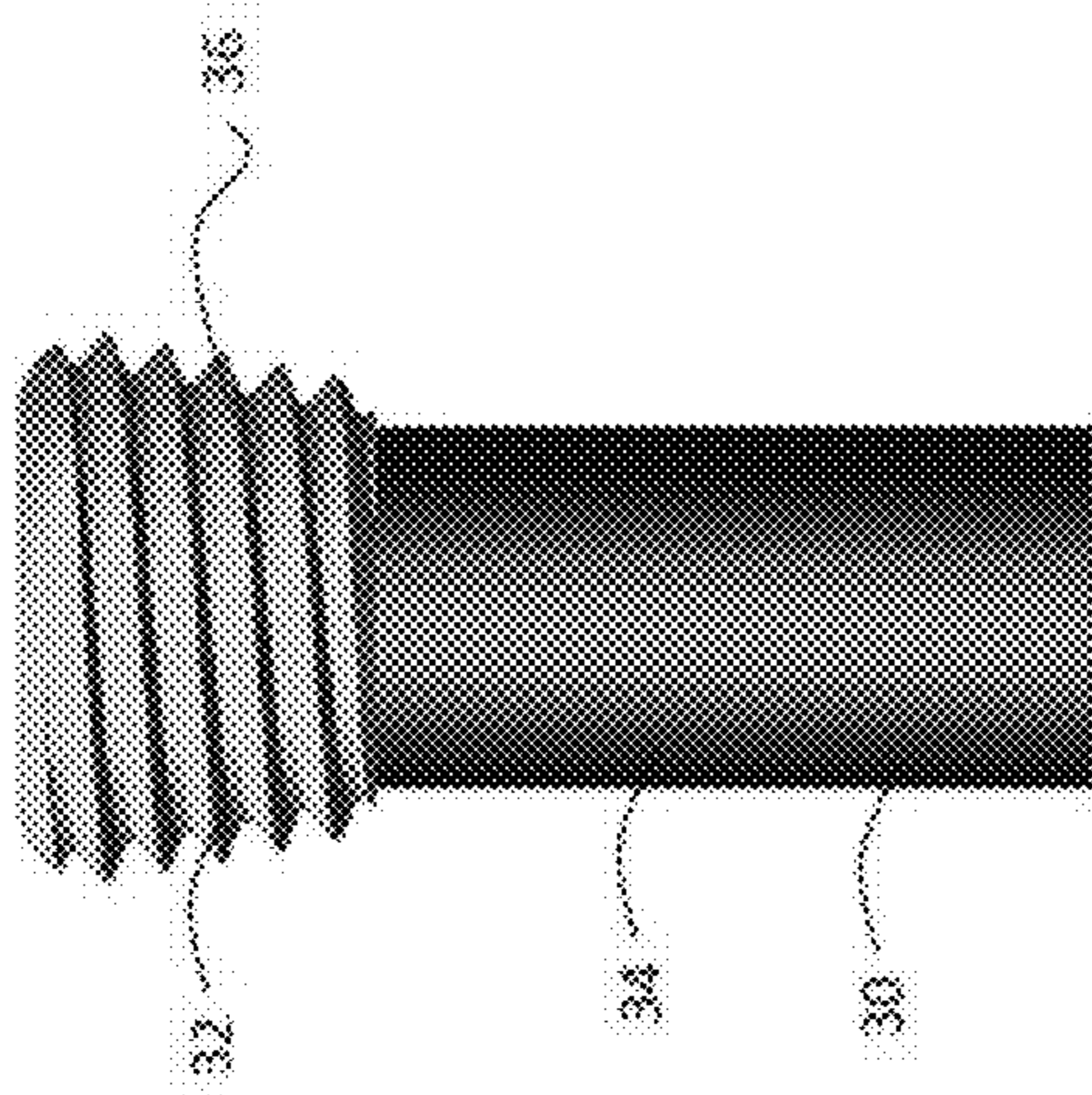


FIG. 13A

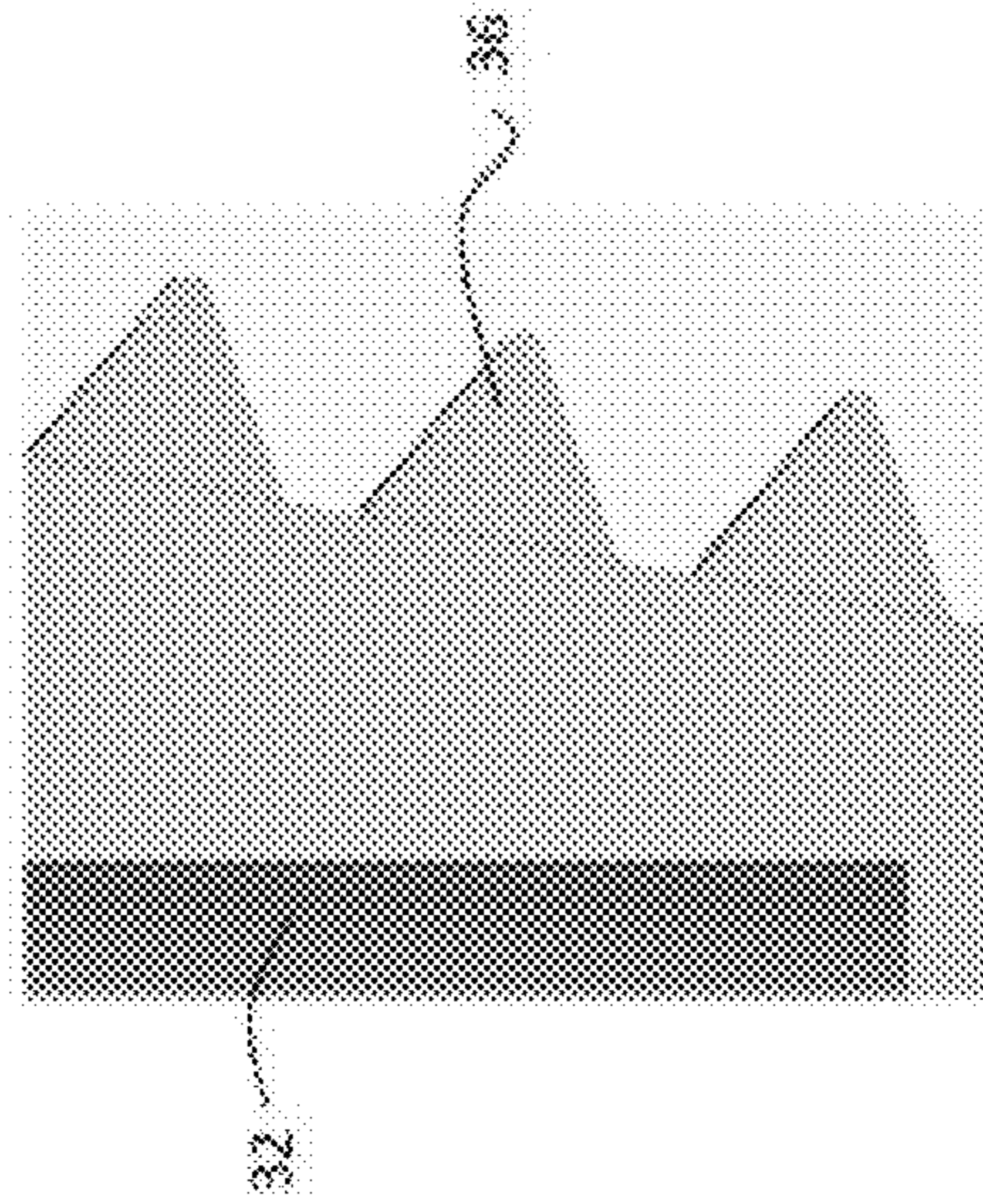


FIG. 13B

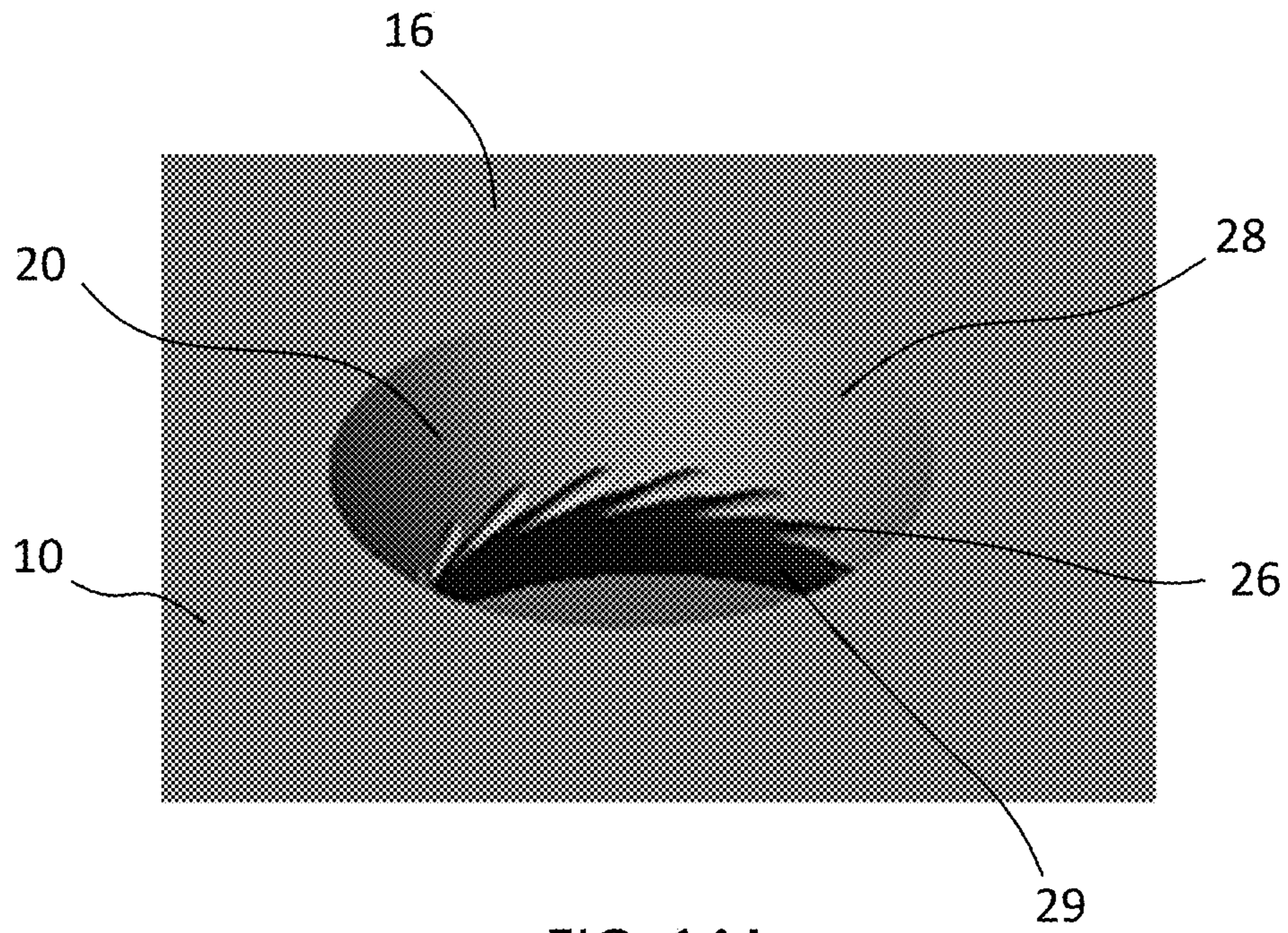


FIG. 14A

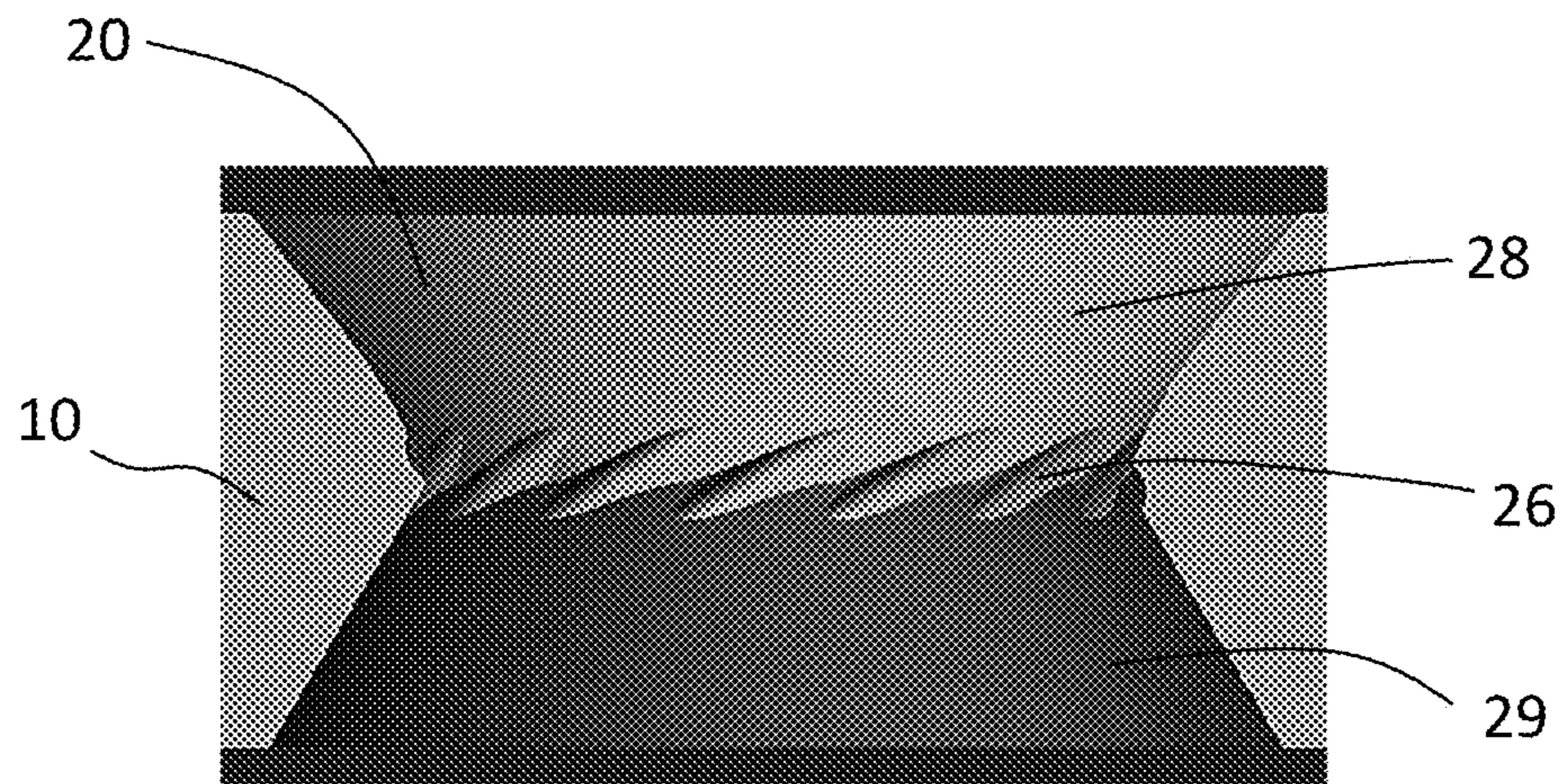


FIG. 14B

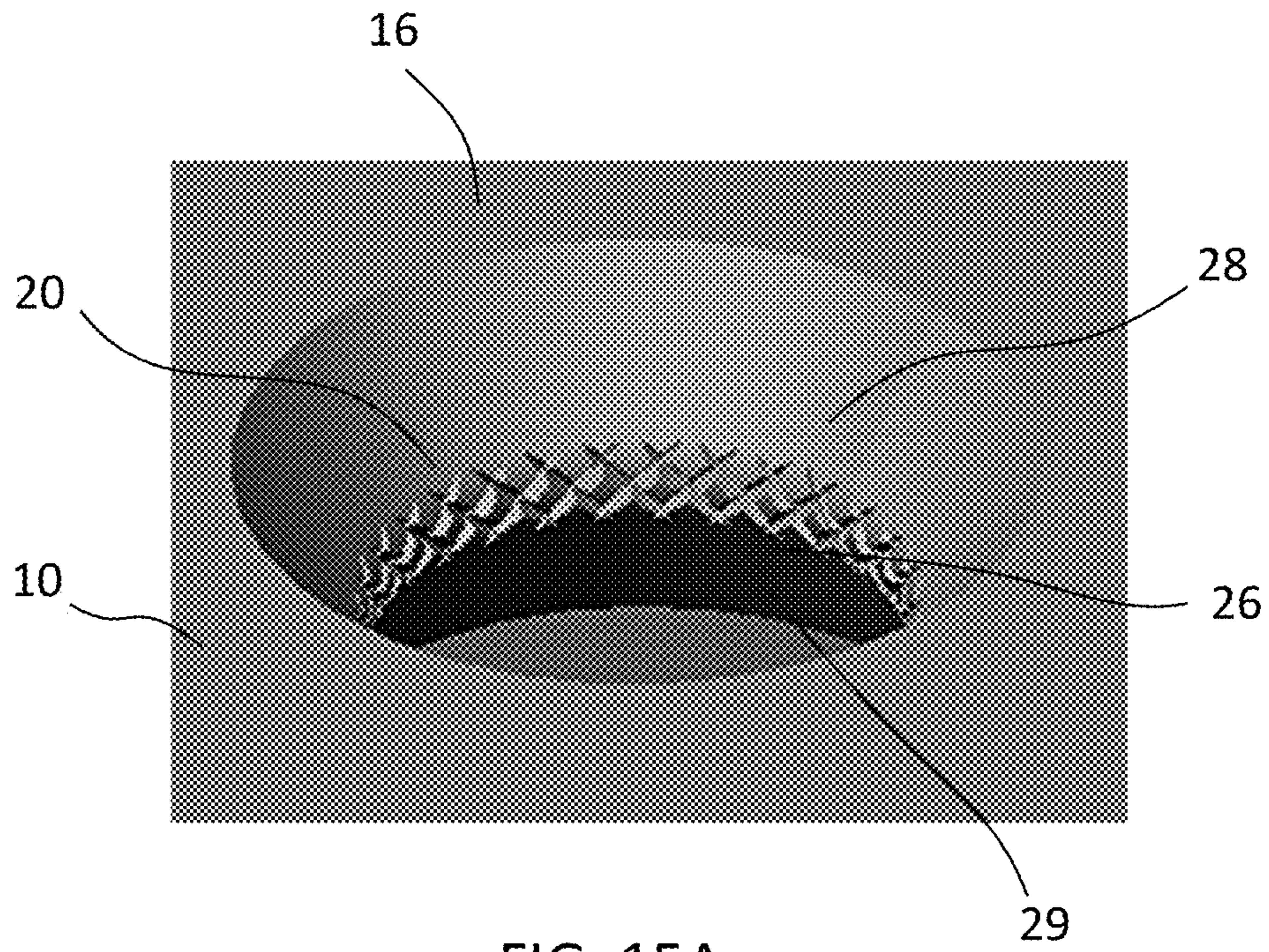


FIG. 15A

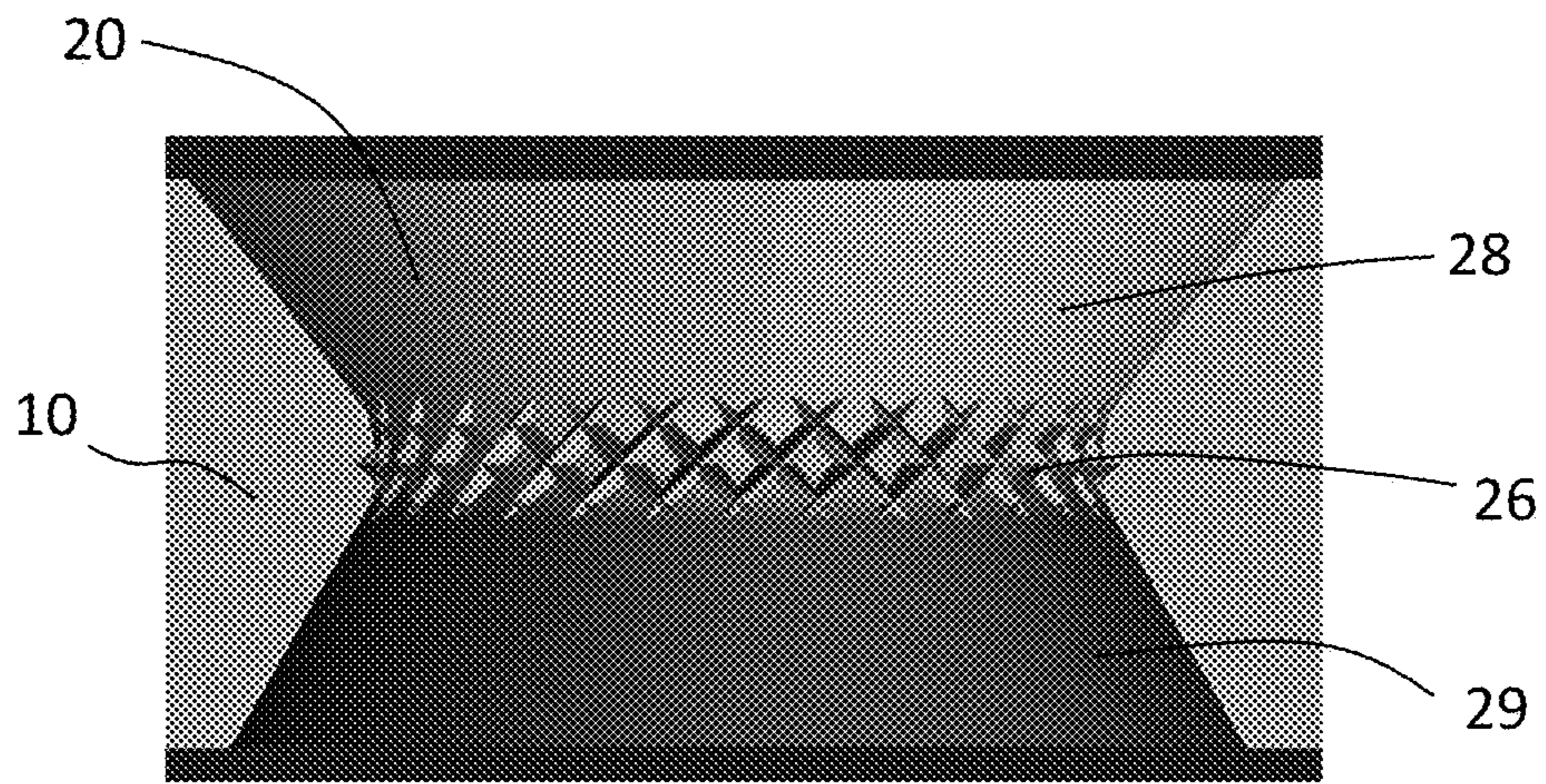


FIG. 15B

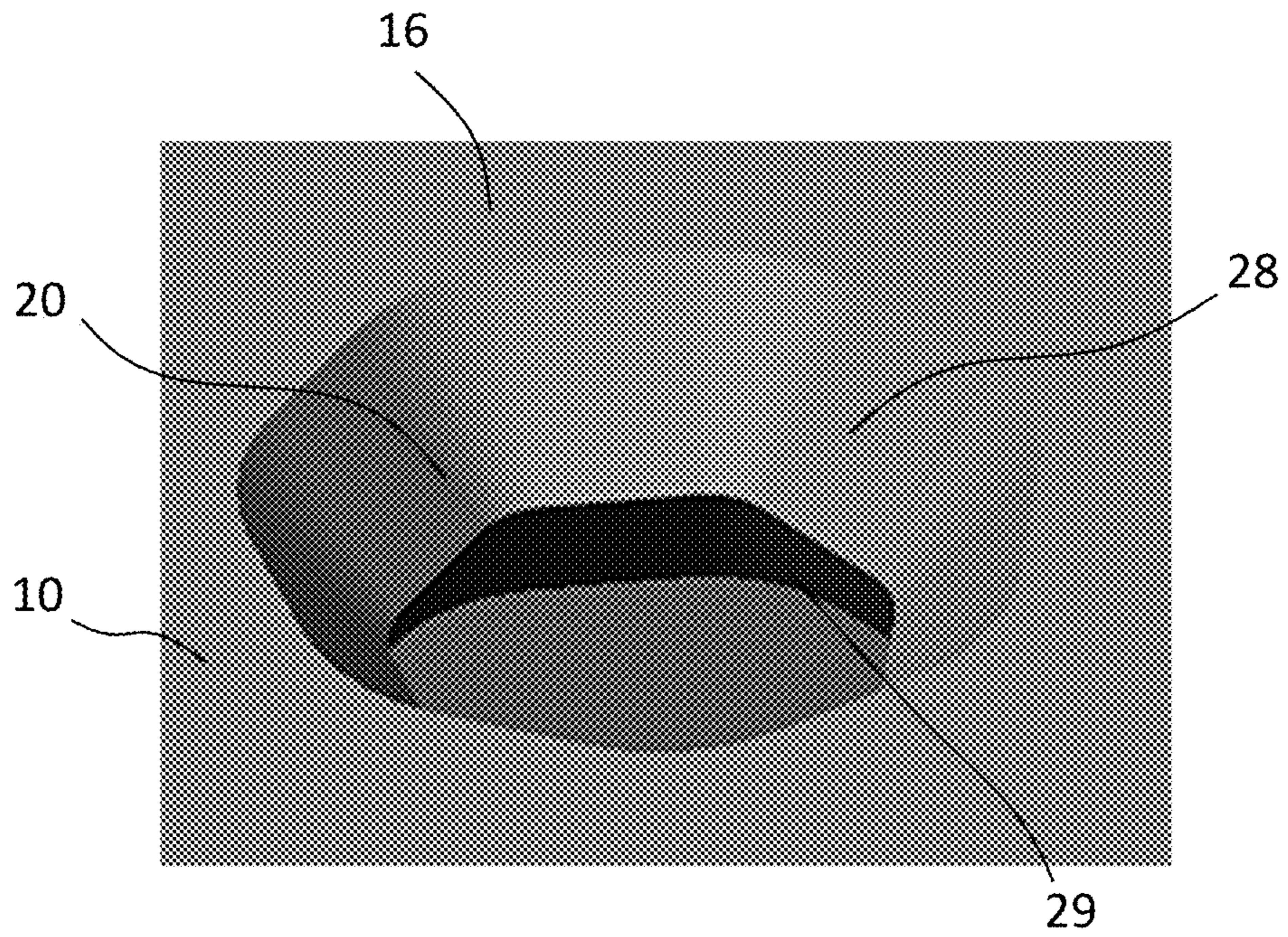


FIG. 16A

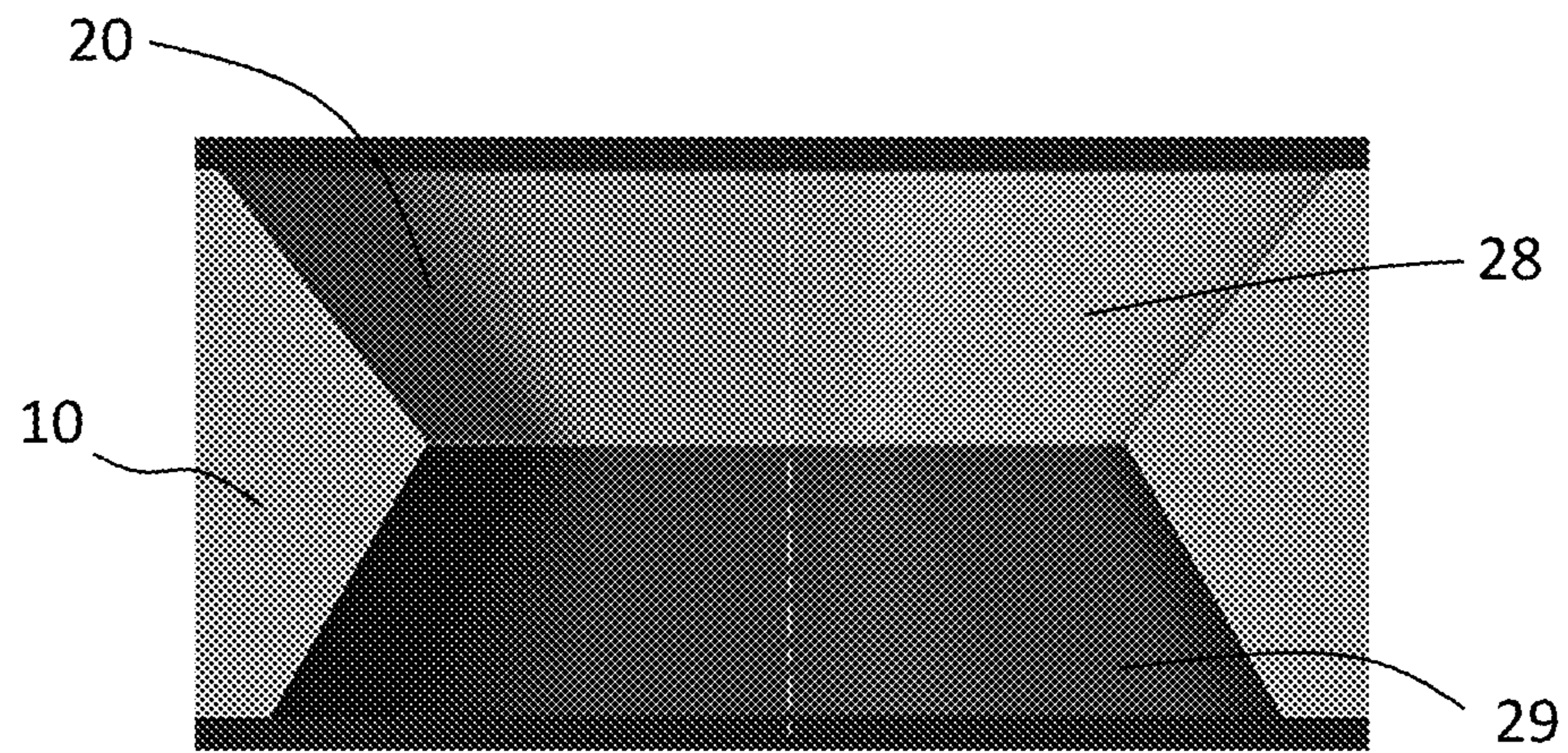


FIG. 16B

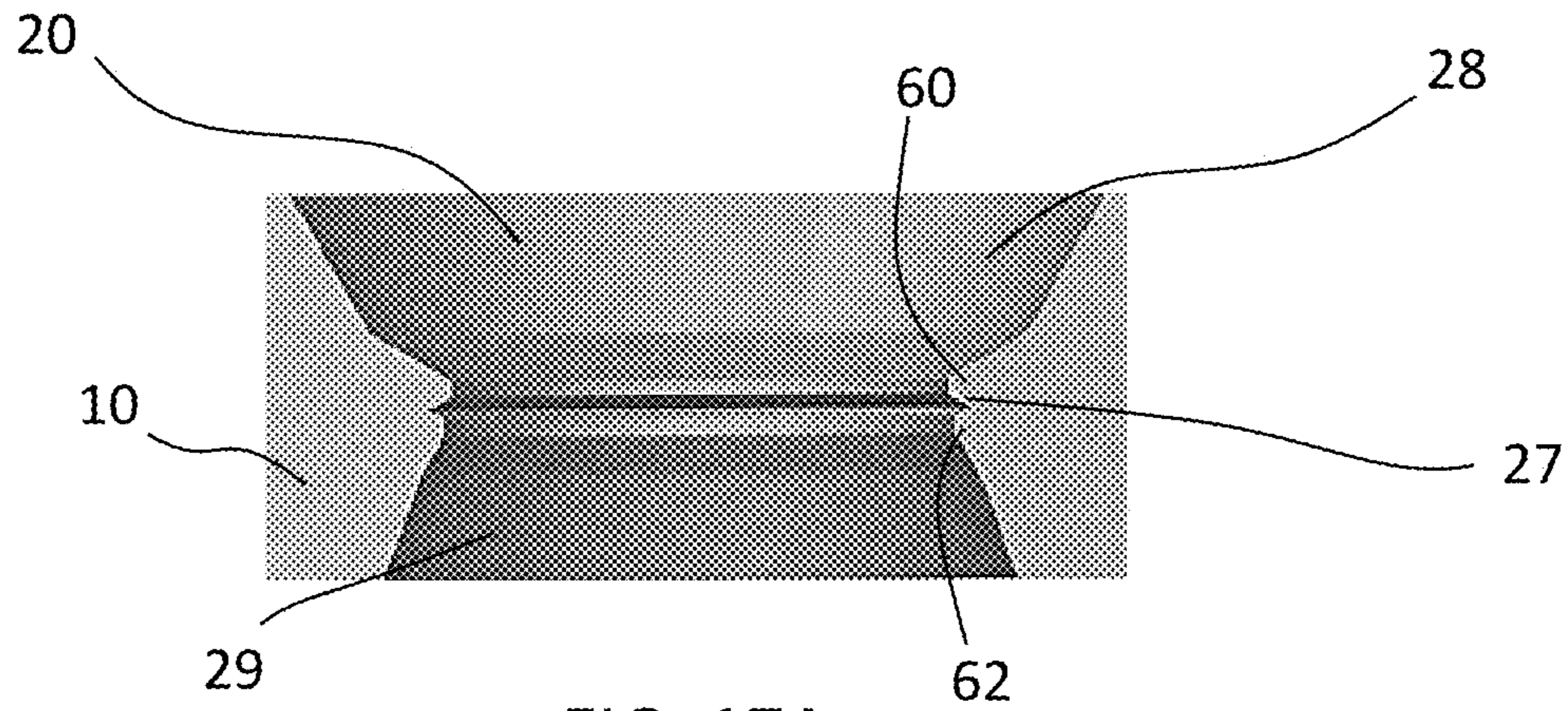


FIG. 17A

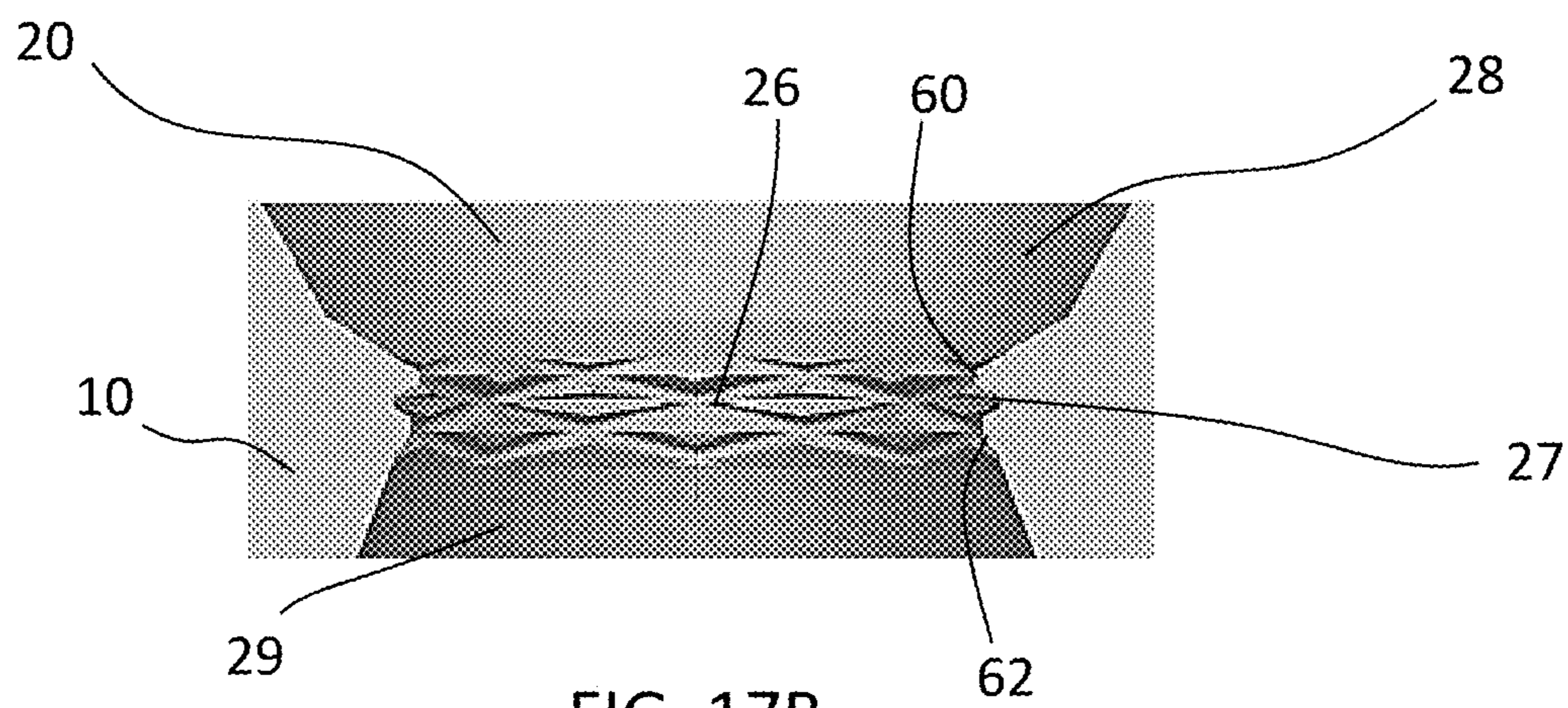


FIG. 17B

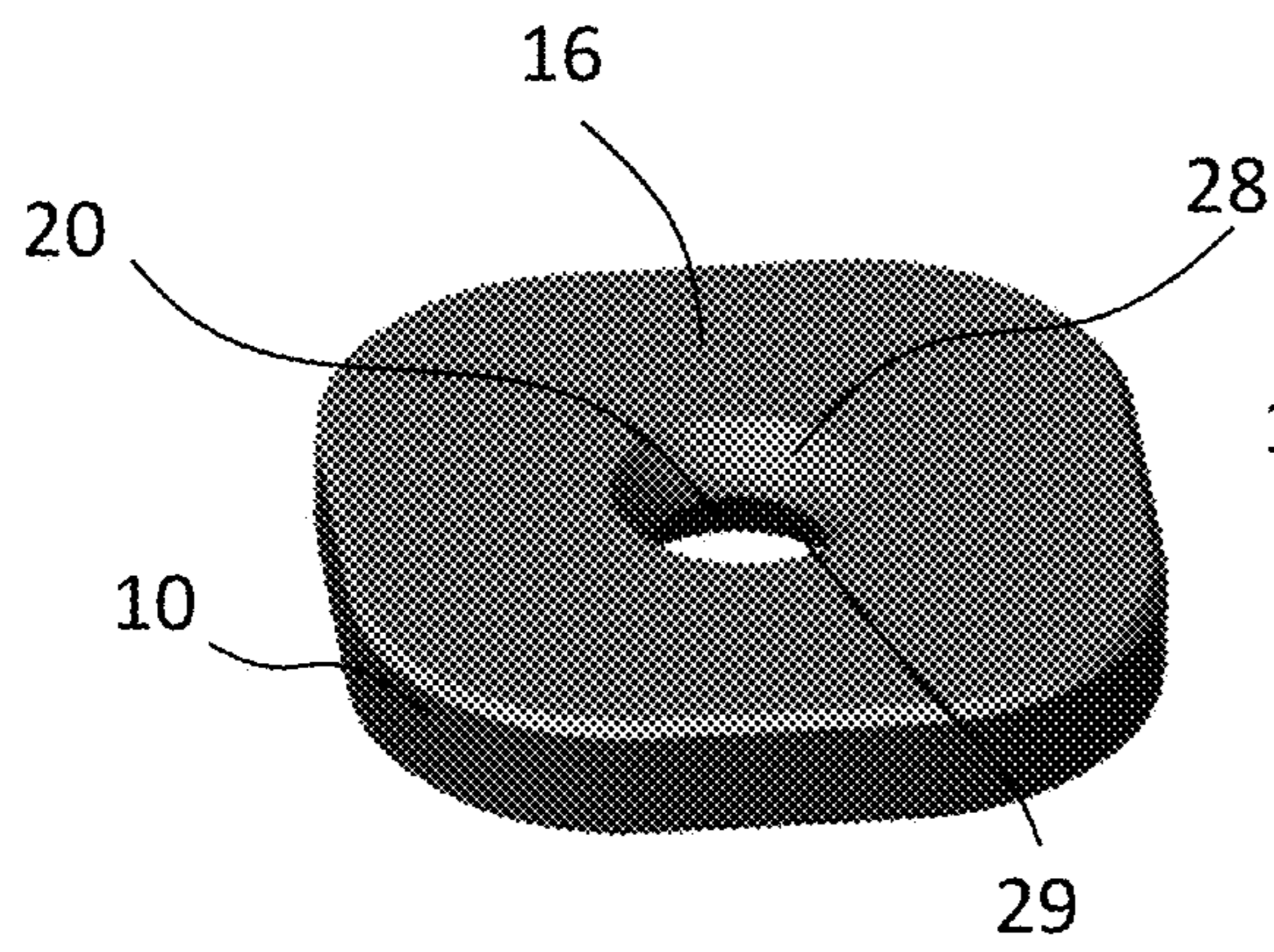


FIG. 18A

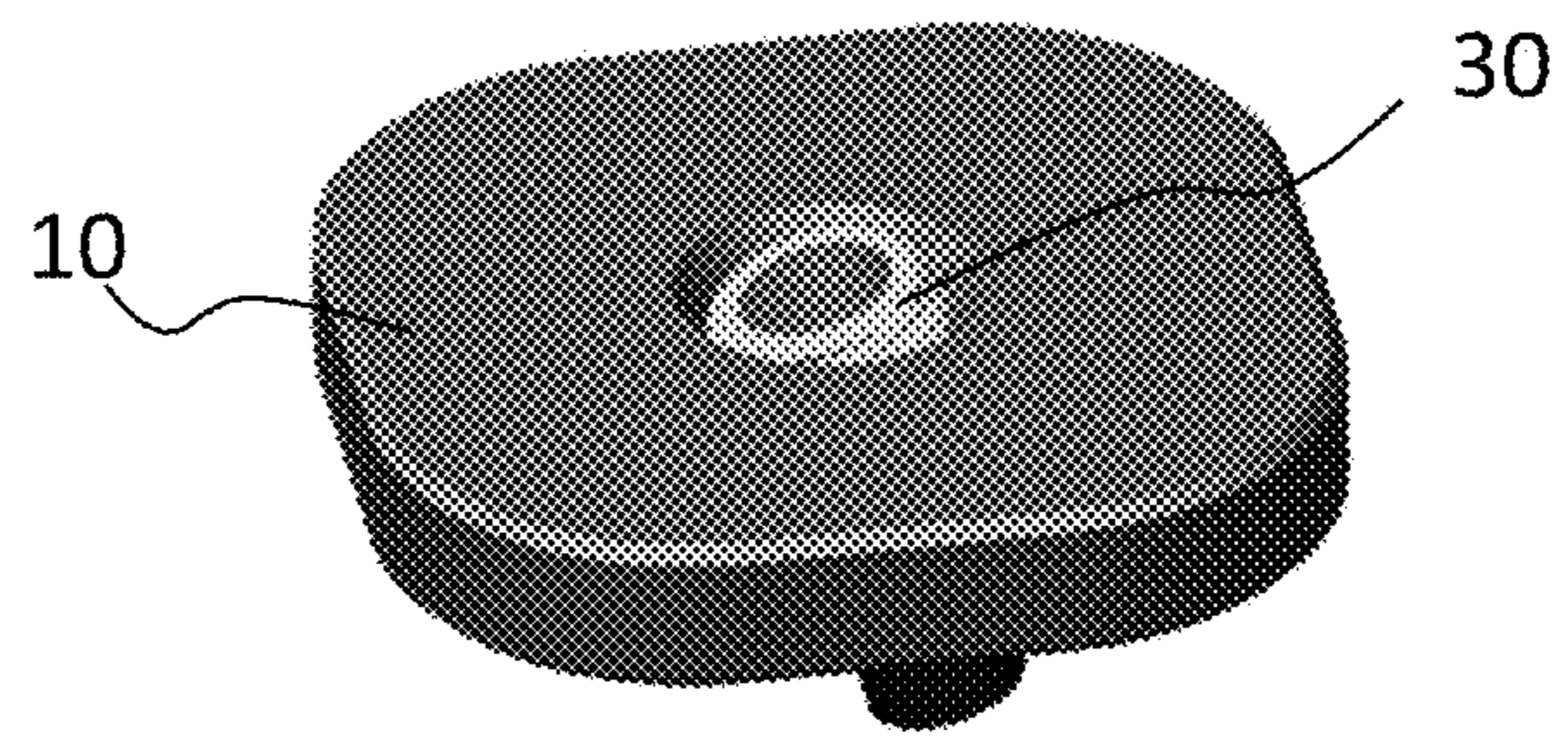


FIG. 18B

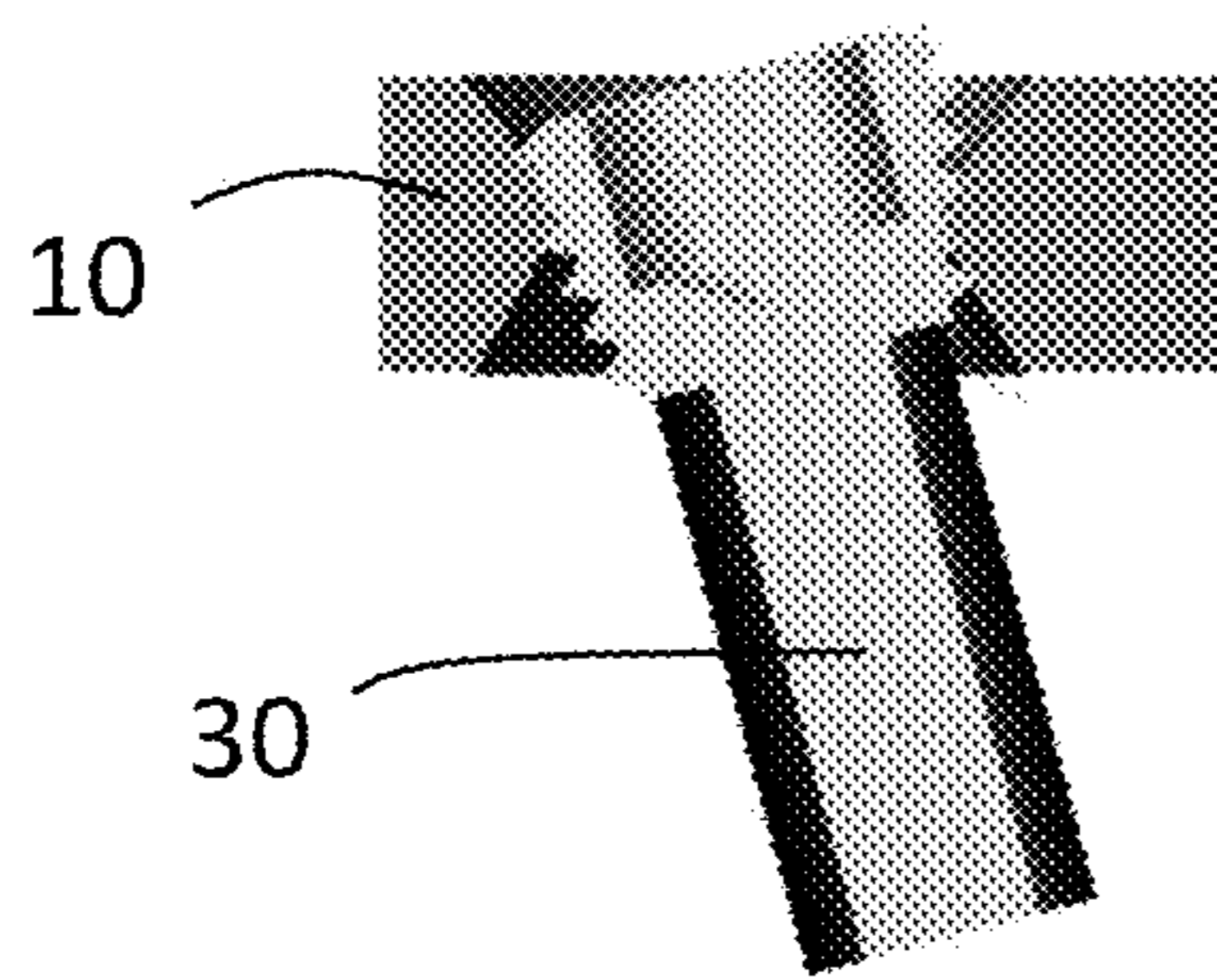


FIG. 18C

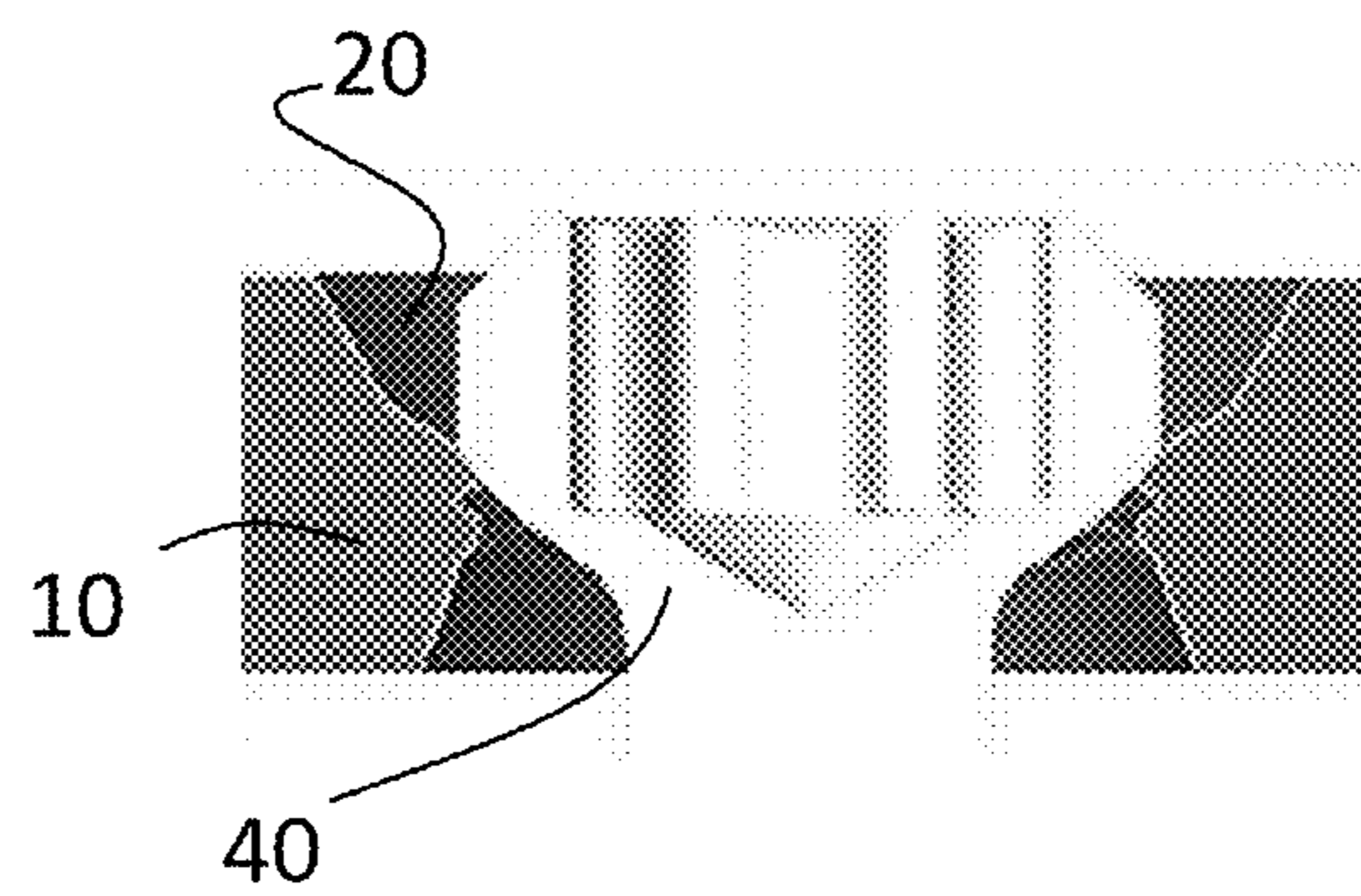


FIG. 18D

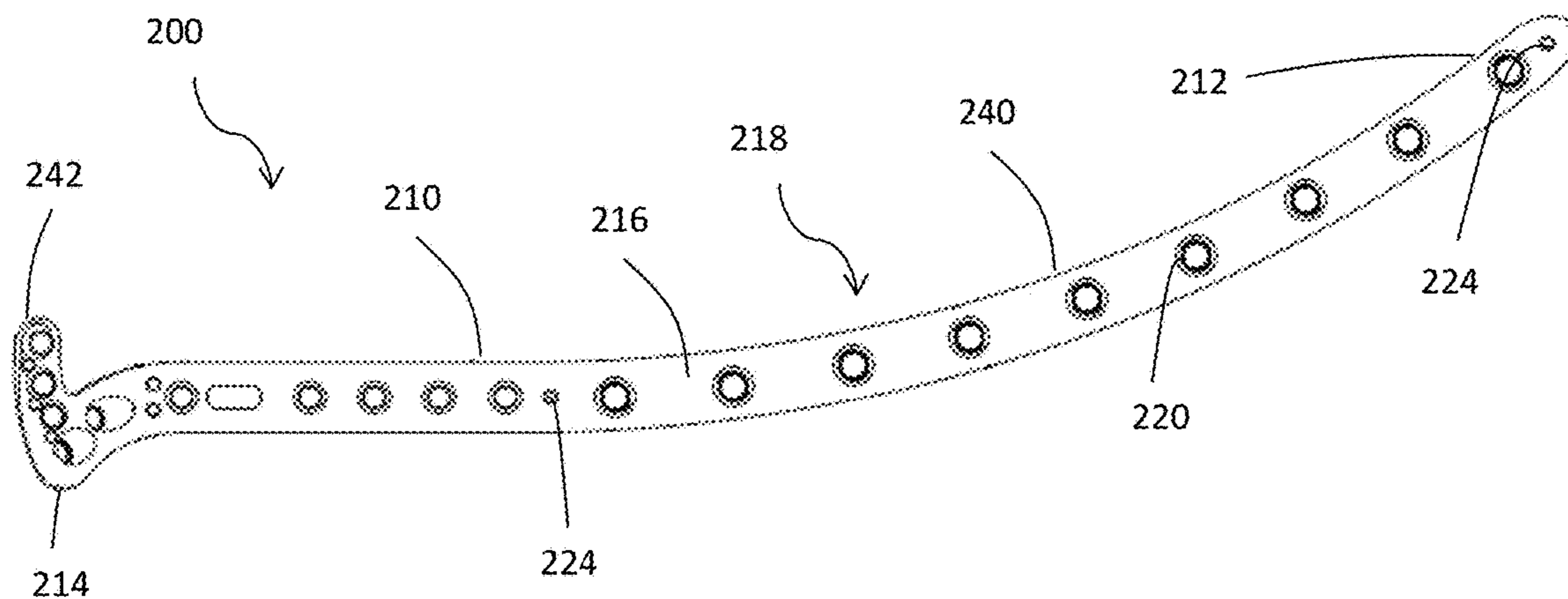


FIG. 19

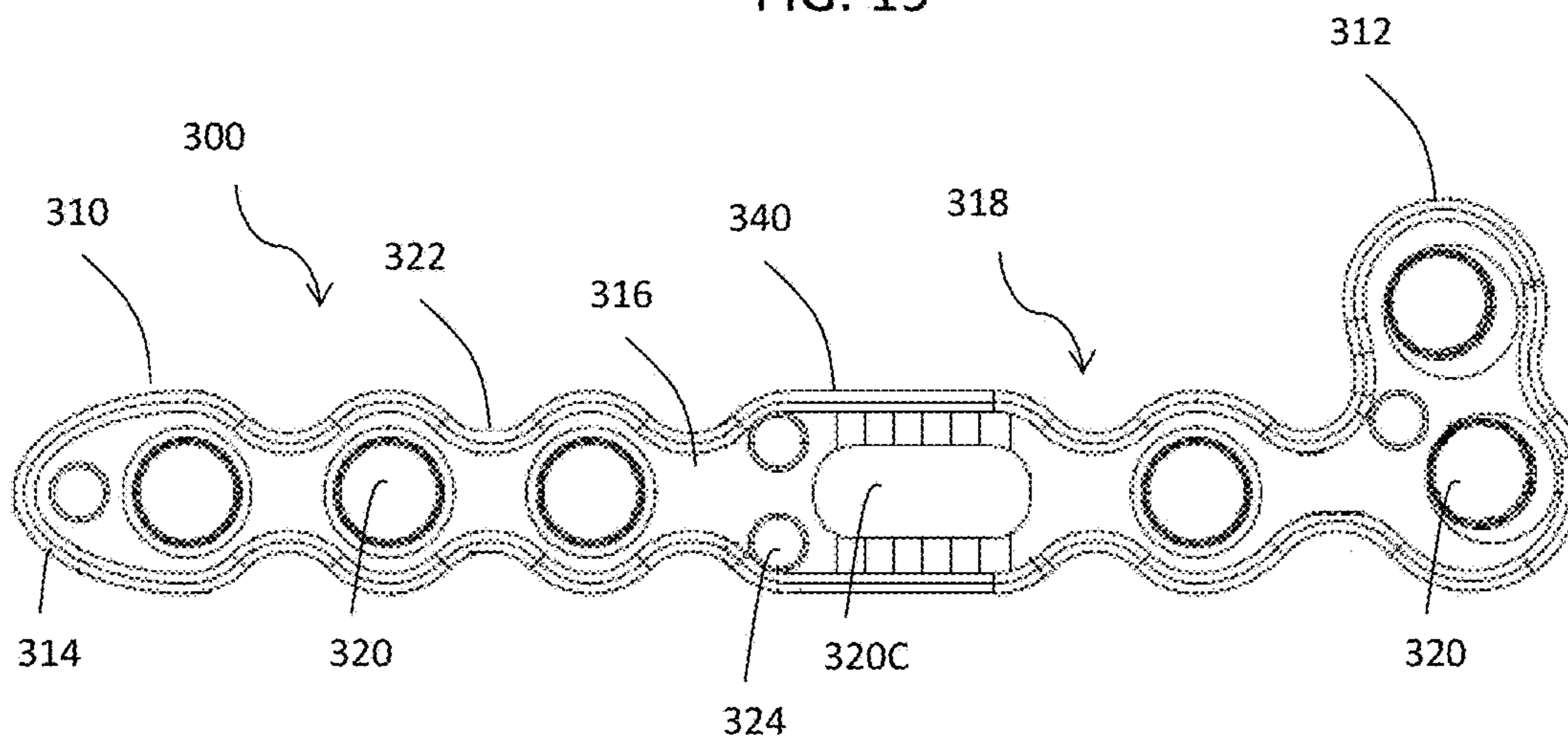


FIG. 20

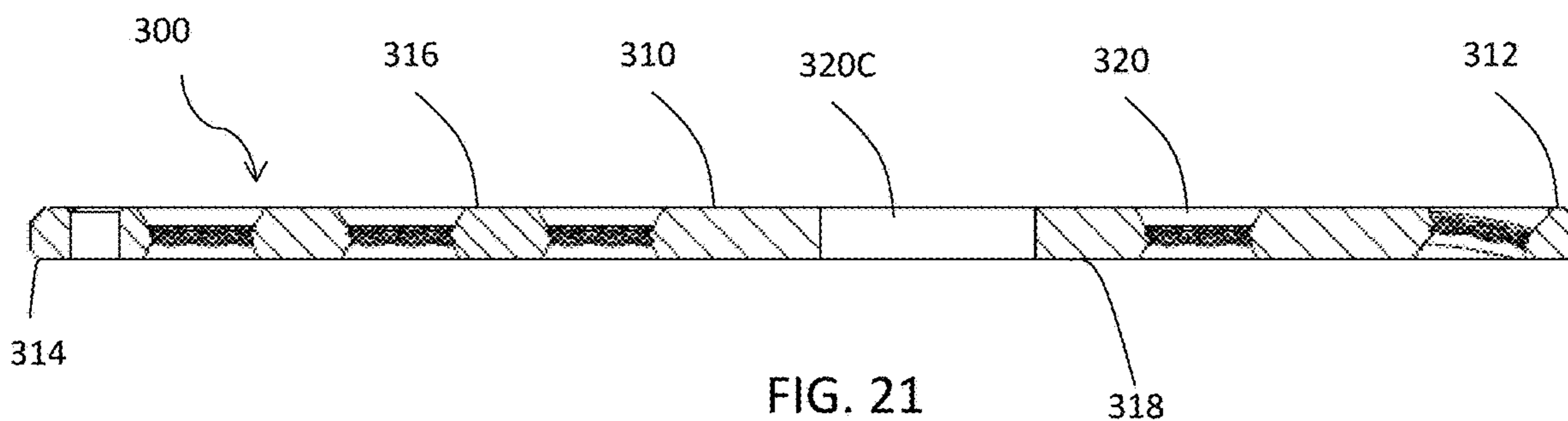


FIG. 21

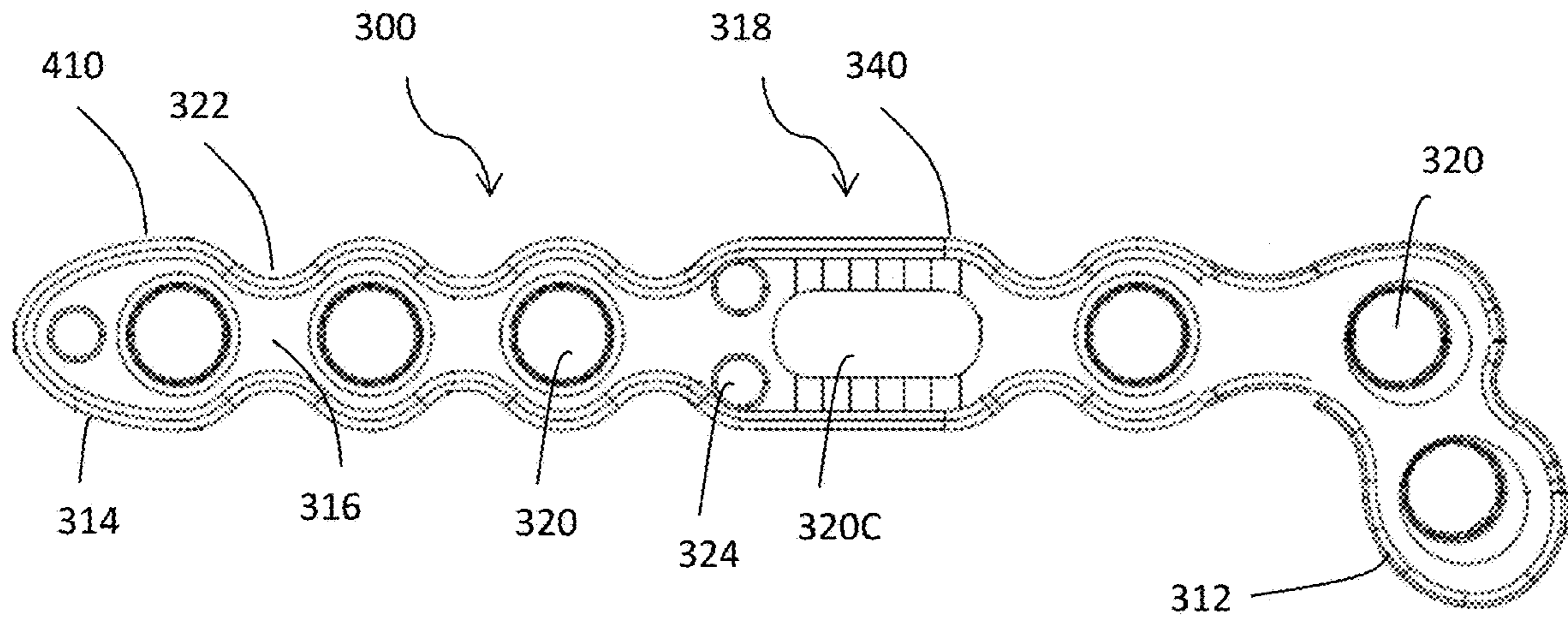


FIG. 22

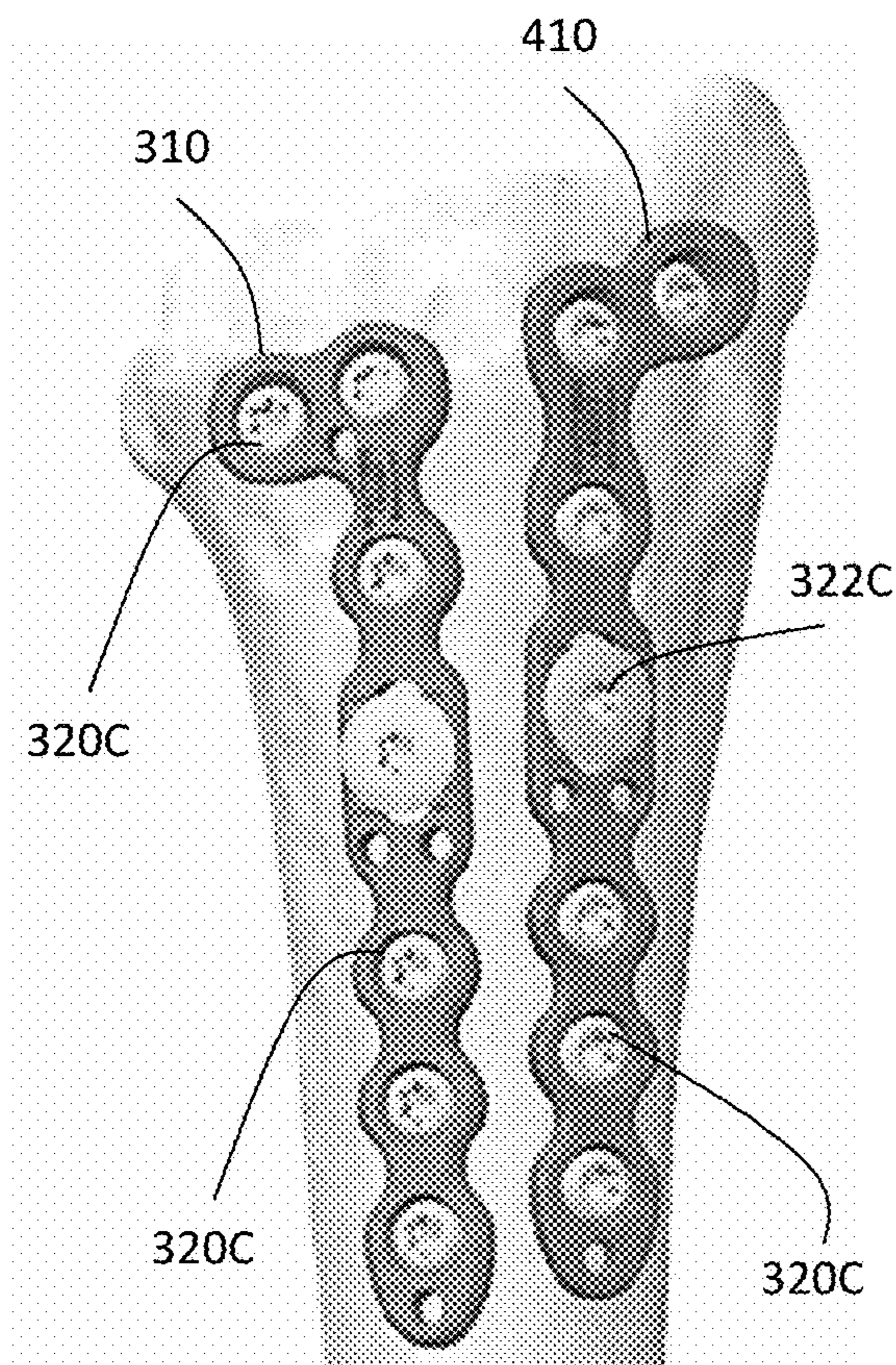


FIG. 23

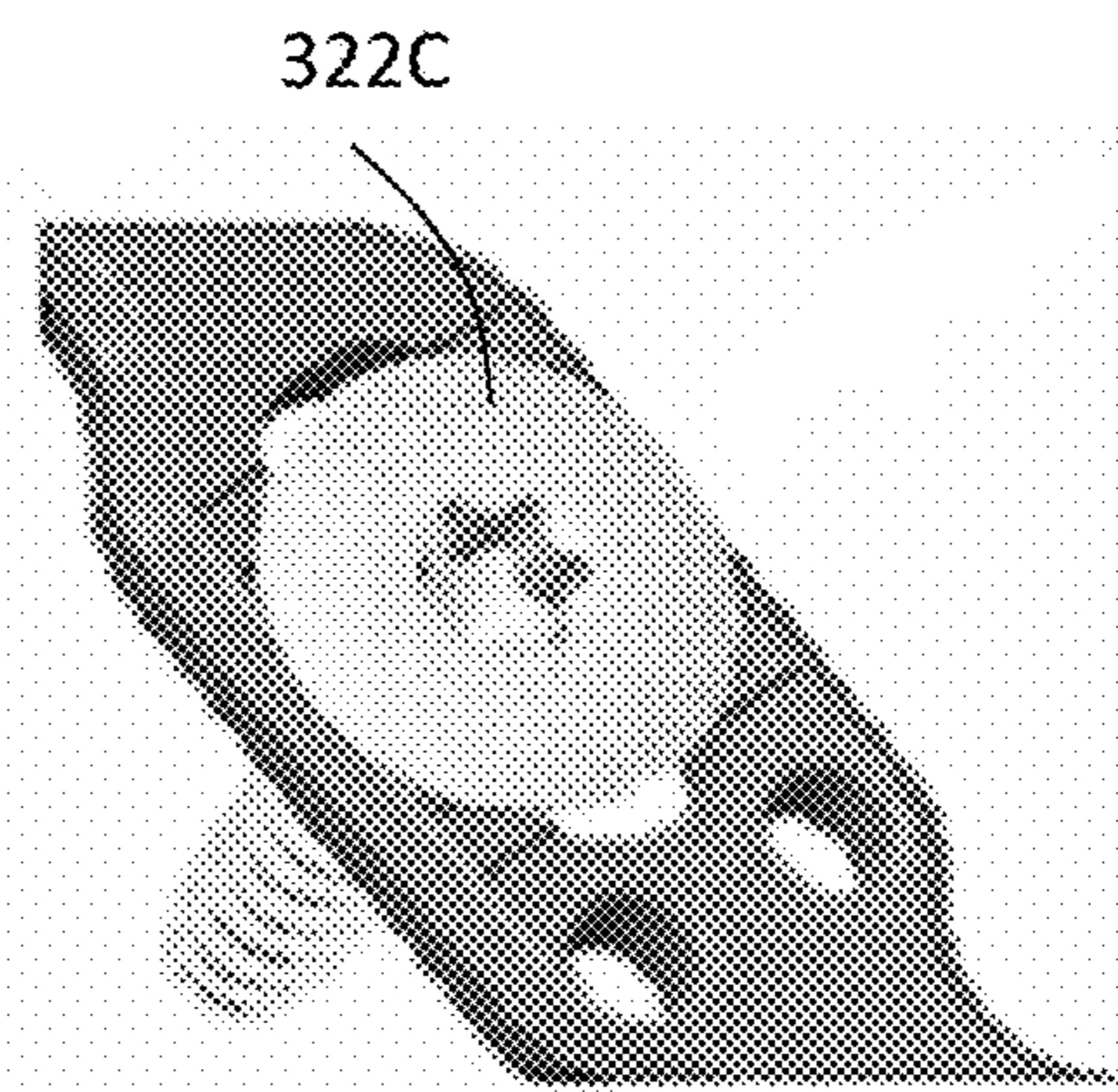


FIG. 24

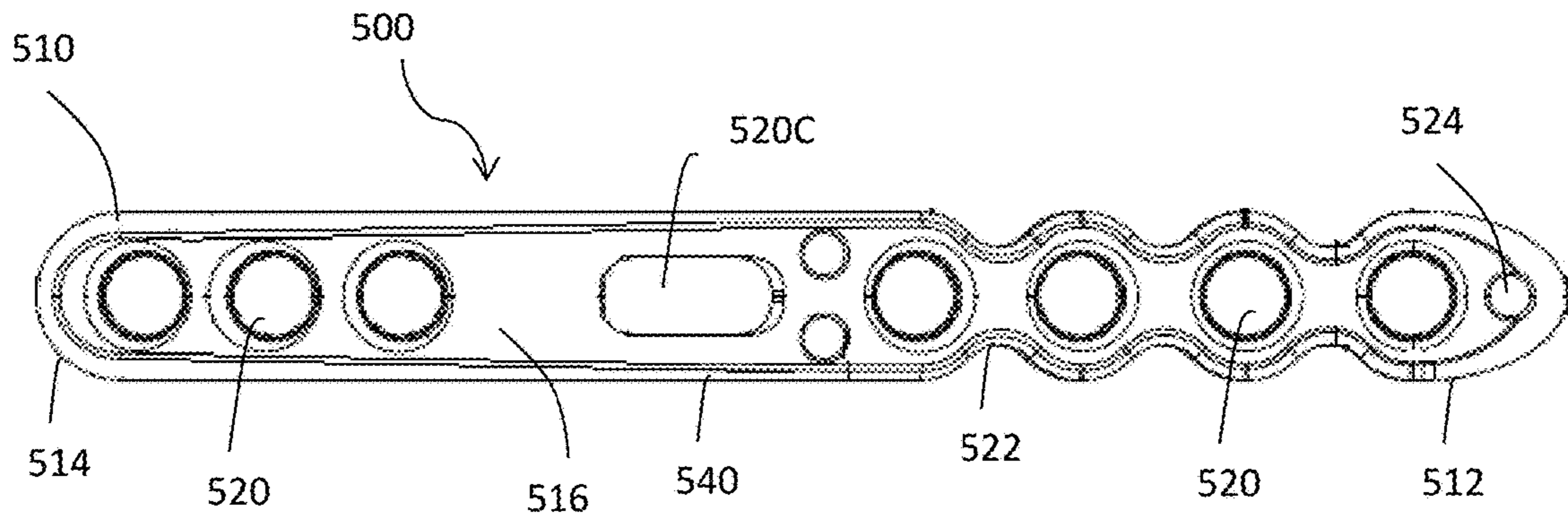


FIG. 25

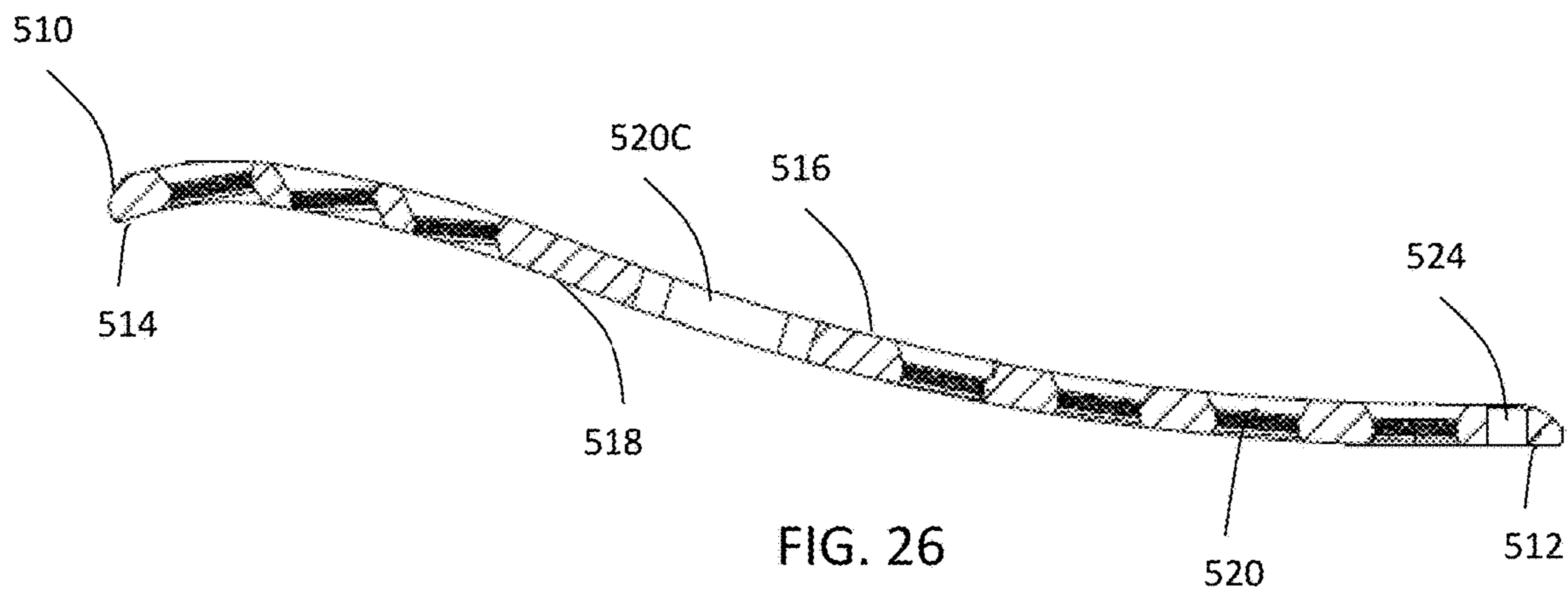


FIG. 26

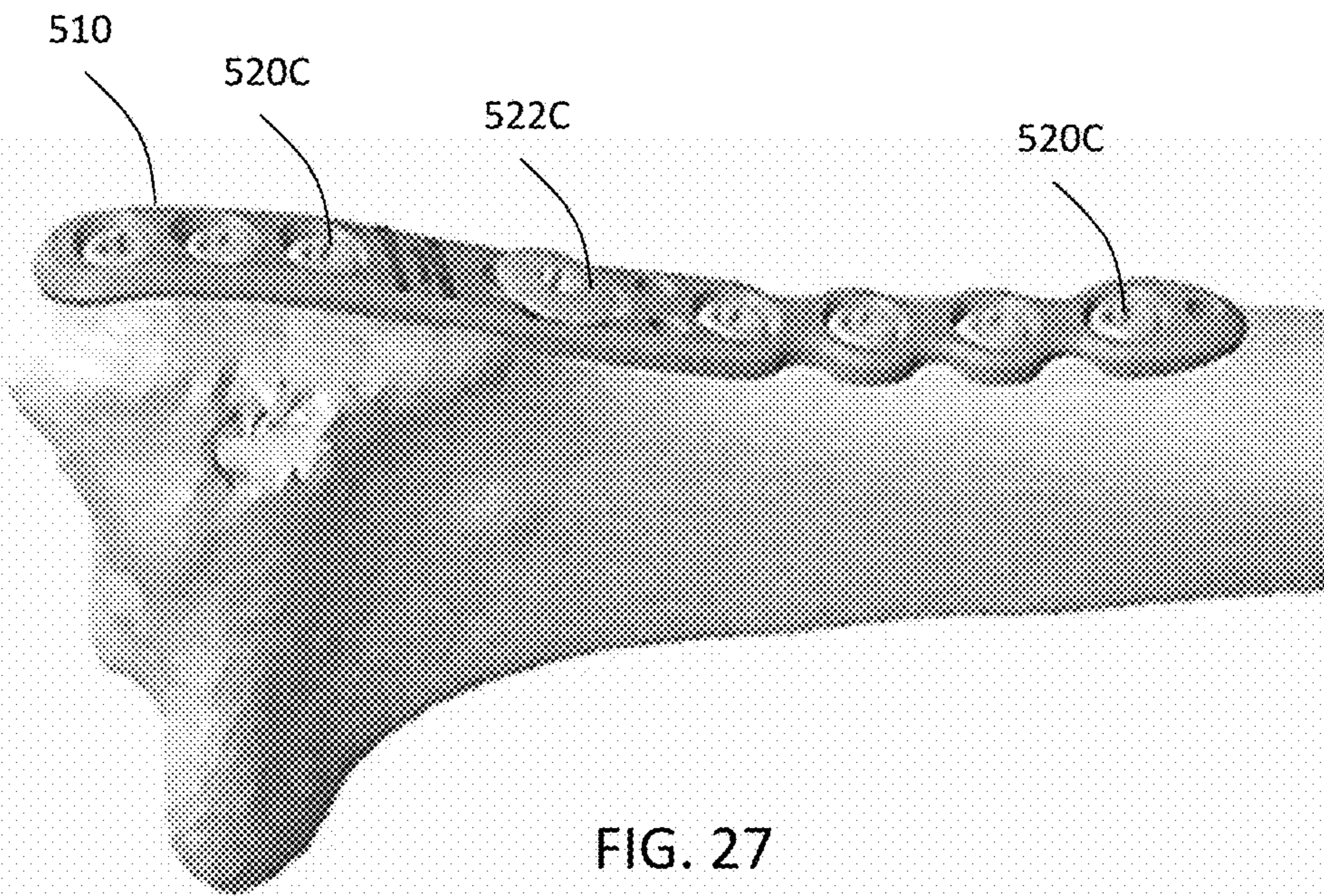


FIG. 27

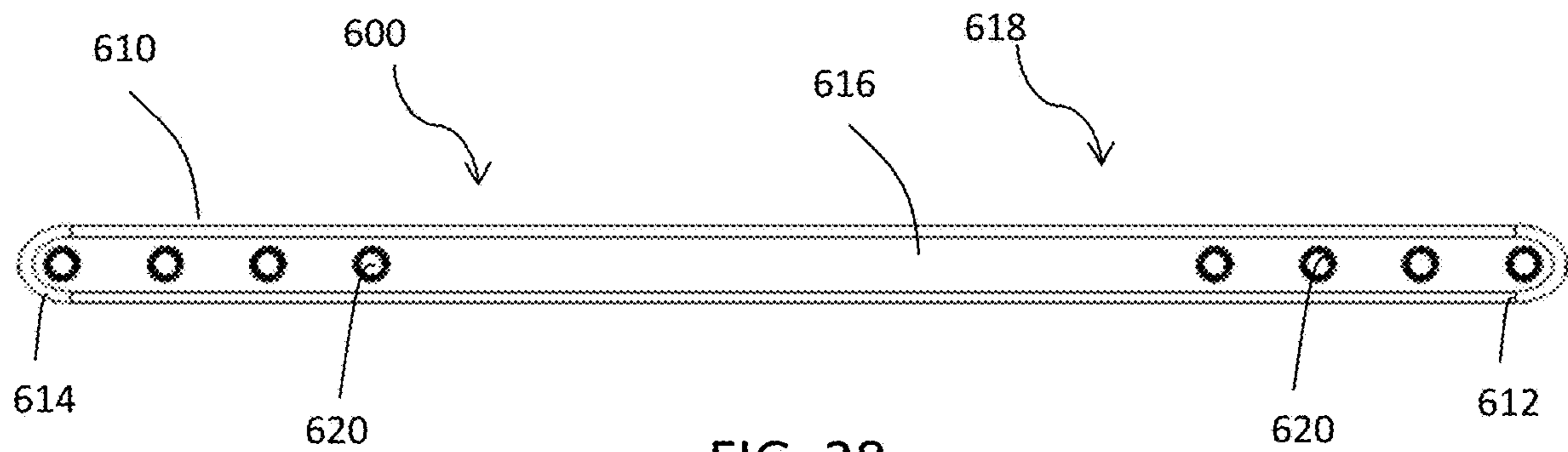


FIG. 28

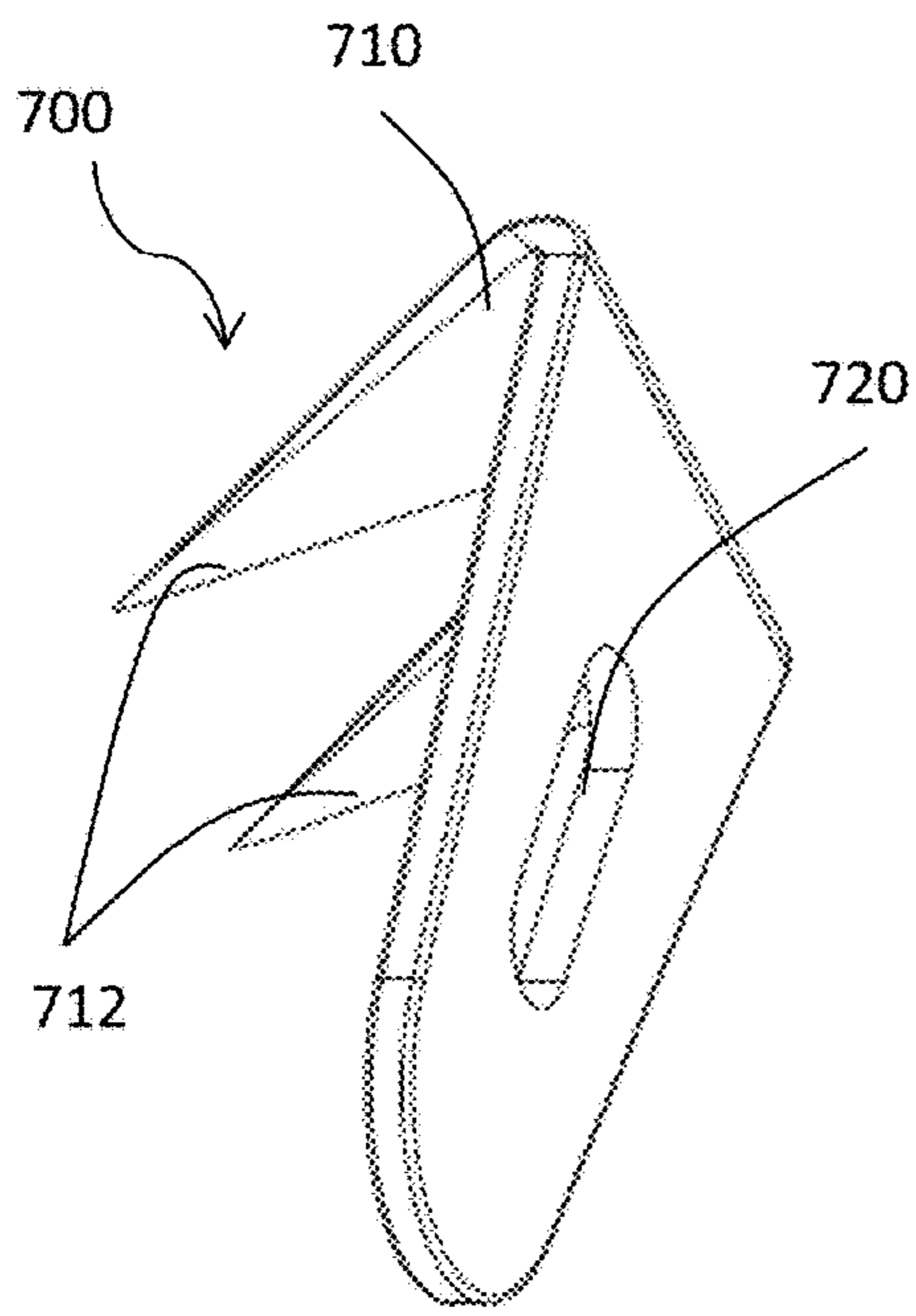


FIG. 29

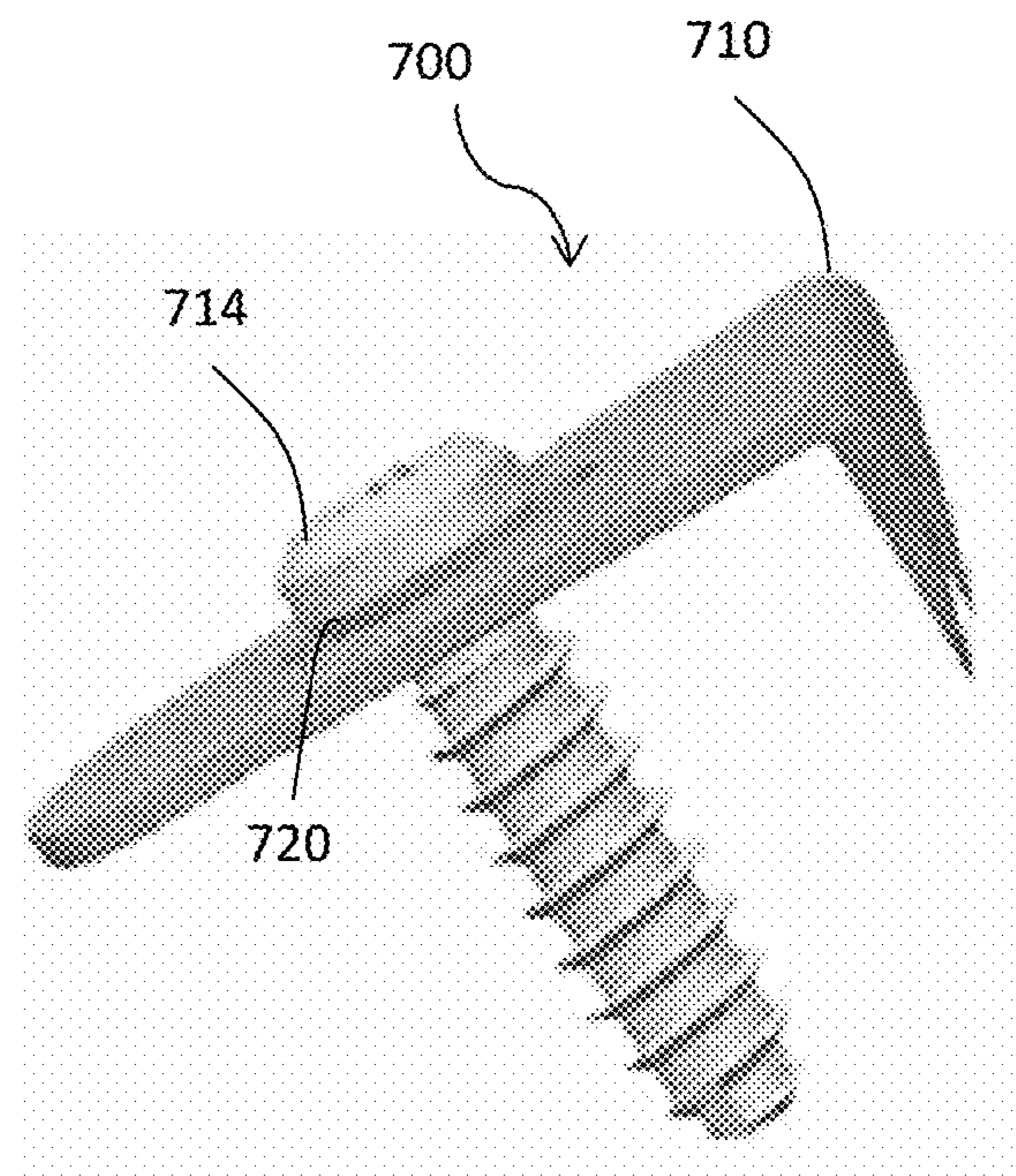


FIG. 30

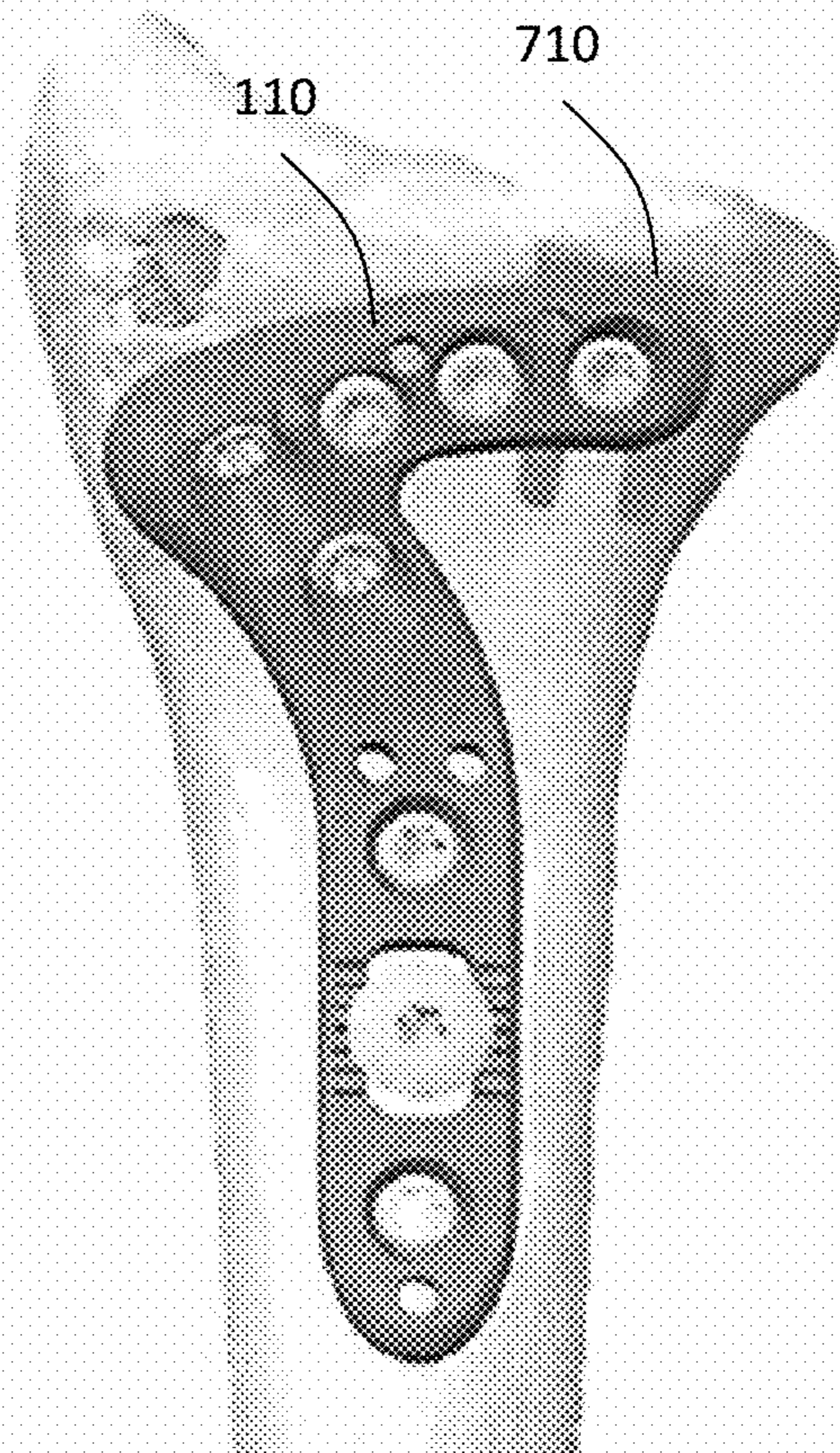


FIG. 31

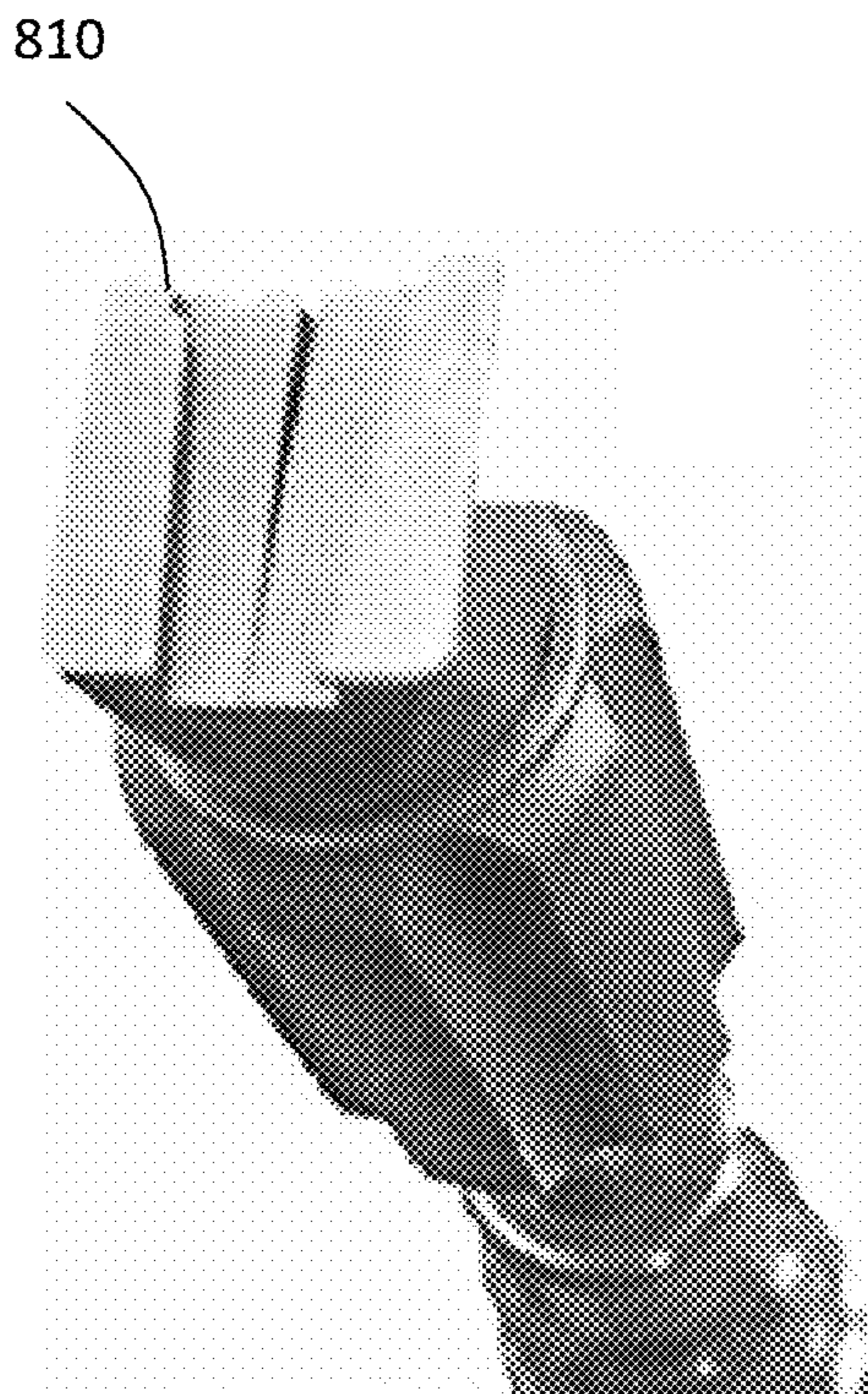


FIG. 32

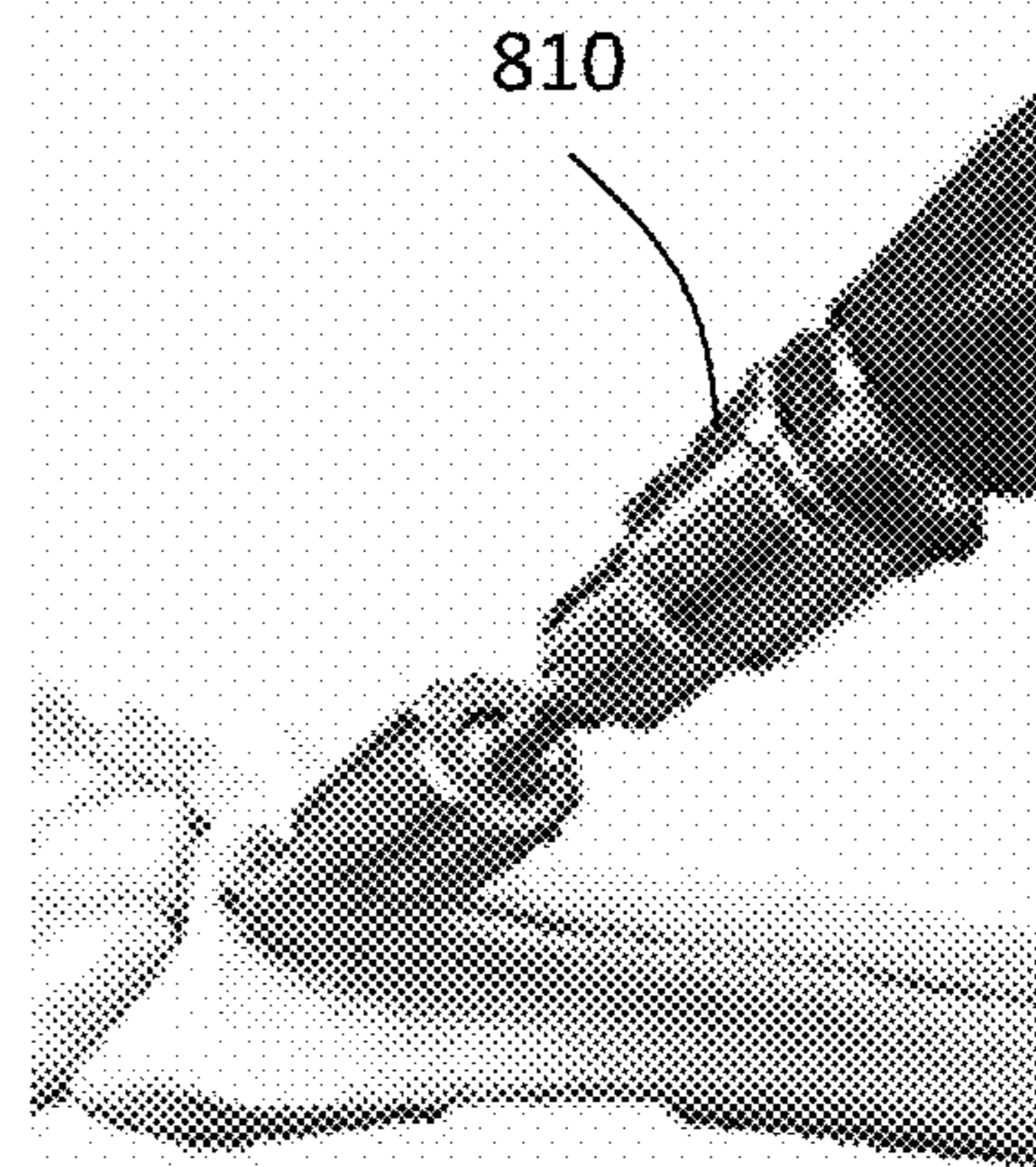


FIG. 33

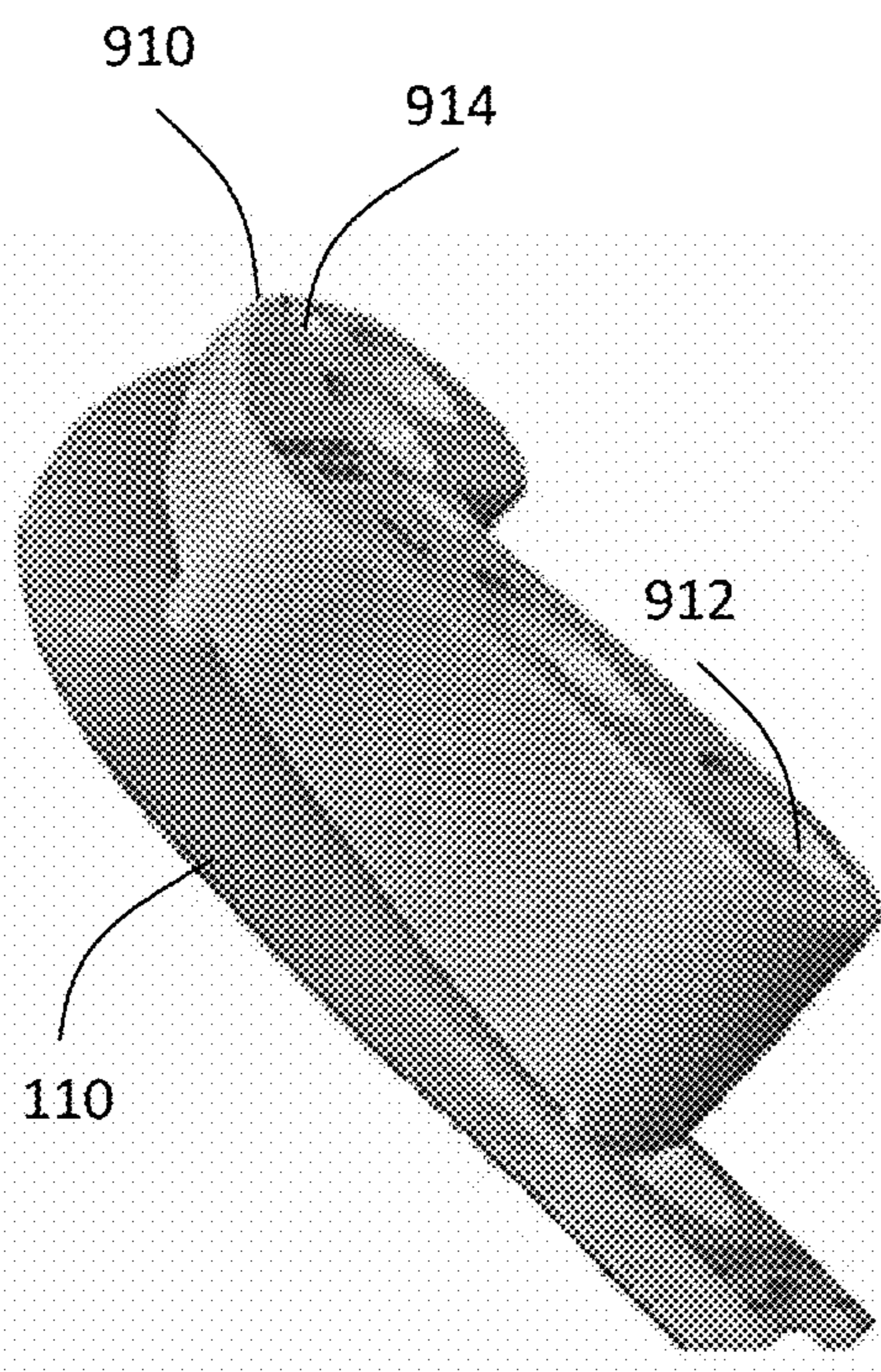


FIG. 34

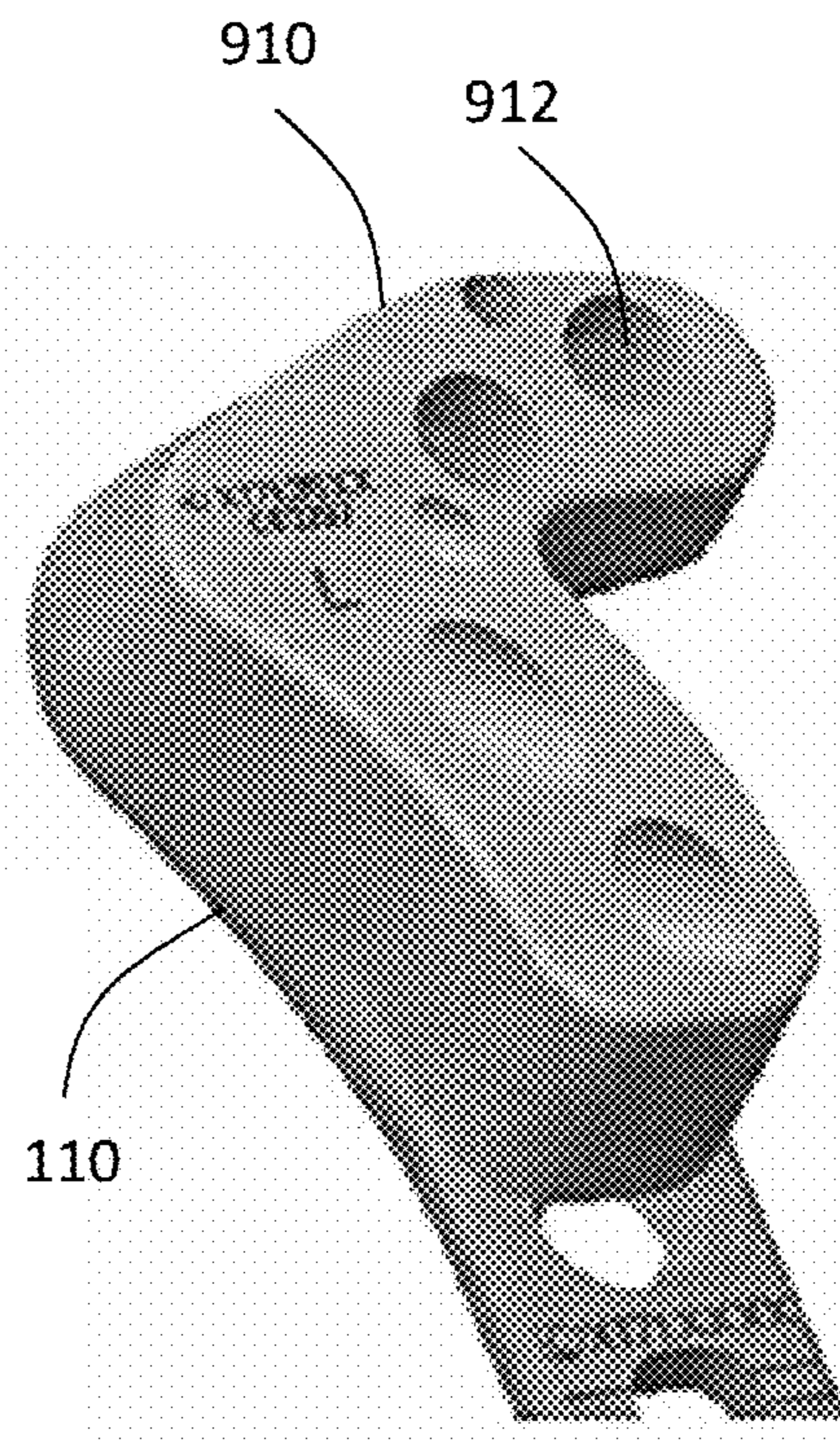


FIG. 35

VOLAR DISTAL RADIUS STABILIZATION SYSTEM

CROSS REFERENCE TO RELATED APPLICATIONS

The present application is Continuation of U.S. patent application Ser. No. 15/456,642, filed on Mar. 13, 2017, which is a Continuation-in-Part of U.S. patent application Ser. No. 15/238,773, filed on Aug. 17, 2016, the contents of which are incorporated herein in their entirety by reference for all purposes.

FIELD

The present disclosure relates to surgical devices and stabilization systems, for example, for trauma applications, and more particularly, for stabilization of volar distal radius fractures.

BACKGROUND

Bone fractures are often repaired by internal fixation of the bone, such as diaphyseal bone, using one or more plates. The plate is held against the fractured bone with screws, for example, which engage the bone and heads which provide a compressive force against the plate. The plate and bone are thus forced against each other in a manner that transfers load primarily between a bone contacting surface of the plate and the bone surface to reinforce the fractured bone during healing. This manner of plating generally creates relatively low stress concentration in the bone, as there may be a large contact area between the plate and the diaphyseal bone surface permitting transfer of load to be dispersed. There may be a desire to use locking screws, non-locking screws, or a combination of both that are able to dynamically compress the bone. Of course, the designs of the plates, types of screws, and locking and/or non-locking capabilities may vary based on the location and type of fracture.

The three long bones of the upper extremity are the humerus, radius, and ulna. In the case of radial fracture fixation, a volar approach may be suitable for plating certain fracture types. There remains a need, however, for improved plating systems for anatomical articular reduction and stable fixation of the radius.

SUMMARY

To meet this and other needs, devices, systems, and methods of bone stabilization are provided, for example, for radius stabilization. The volar distal radius stabilization systems may include one or more plates and one or more fasteners. Although generally described with reference to the radius, it will be appreciated that the stabilization systems described herein may be used or adapted to be used for the fixation of other long bones as well, such as the humerus, femur, tibia, etc.

According to one embodiment, a stabilization system includes a bone plate and a plurality of fasteners. The bone plate comprises an elongated portion extending along a longitudinal axis, an enlarged head portion, and a transition region connecting the elongated portion to the enlarged head portion, wherein the transition region is curved and connect to an end portion of the enlarged head portion, the bone plate comprising a plurality of through holes extending through the enlarged head portion, the transition region, and the elongated portion. The fasteners are configured to extend

through one or more of the plurality of through holes in the bone plate and configured to secure the bone plate to the bone.

The fasteners may include locking fasteners (e.g., configured to lock to the plate), non-locking fasteners (e.g., configured to provide dynamic compression of the bone), polyaxial fasteners (e.g., configured to be inserted at a plurality of angles or trajectories), fixed angle fasteners (e.g., configured to be inserted at a fixed angle or trajectory), or any other suitable fasteners known in the art.

In some instances, the locking fasteners may include fasteners having self-forming threads on a head portion of the fasteners, which are configured to lock to at least one of the plurality of through holes on the plate.

According to another embodiment, a stabilization system configured to stabilize a radius includes a bone plate, a plurality of fixed angle fasteners, a polyaxial fastener, and a fastener. The bone plate comprises an elongated portion extending along a longitudinal axis, an enlarged head portion, and a transition region connecting the elongated portion to the enlarged head portion, wherein the transition region is curved and connect to an end portion of the enlarged head portion, the bone plate comprising a plurality of fixed angle holes positioned in general alignment along the elongated portion, a polyaxial hole positioned proximate to the end portion of the enlarged head portion connected to the transition region, and an elongated slot on the elongated portion. The fixed angle fasteners are configured to be received in the fixed angle holes, the plurality of fixed angle fasteners configured to be aimed at a radio-carpal joint and a distal radio-ulnar joint. The polyaxial fastener is configured to be received in the polyaxial hole, the polyaxial fastener configured to be aimed at a radial styloid. The fastener is configured to be received in the elongated slot, wherein the elongated slot allows for proximal-distal and medial-lateral adjustment of the plate.

According to another embodiment, a stabilization system for stabilizing a bone includes a bone plate and a plurality of fasteners. The bone plate has an upper surface and a lower surface configured to contact the bone, wherein the lower surface comprises one or more recesses configured to reduce contact between the plate and a surface of the bone. The bone plate comprises an elongated portion extending along a longitudinal axis, an enlarged head portion, and a transition region connecting the elongated portion to the enlarged head portion, wherein the transition region is connect to an end portion of the enlarged head portion and the other end portion of the enlarged head portion is a free end, the bone plate comprising a plurality of through holes extending through the enlarged head portion, the transition region, and the elongated portion. The plurality of fasteners are configured to extend through one or more of the plurality of through holes in the bone plate and configured to secure the bone plate to the bone.

According to yet another embodiment, one or more methods of installing a stabilization system may include aligning a bone plate against the volar side of the radial bone, and inserting one or more fasteners through the bone plate and into the bone to stabilize the radius and repair the fracture.

Also provided are kits for the stabilization systems including bone plates of varying sizes and orientations, fasteners including locking fasteners, non-locking, compression fasteners, polyaxial fasteners, fixed angle fasteners, or any other suitable fasteners, drill guides, k-wires, and other components for installing the same.

BRIEF DESCRIPTION OF THE DRAWINGS

A more complete understanding of the present invention, and the attendant advantages and features thereof, will be

more readily understood by reference to the following detailed description when considered in conjunction with the accompanying drawings wherein:

FIGS. 1A-1J depict stabilization systems according to embodiments including volar distal radius bone plates and a plurality of bone fasteners;

FIG. 2 is a top perspective view of two fasteners engaged with combination holes according to an embodiment;

FIG. 3 is a close-up view of an alternative version of a combination hole according to another embodiment;

FIGS. 4A-4C show a perspective view, top view, and cross-section view, respectively, of an another embodiment of a combination hole;

FIGS. 5A-5C show a perspective view, top view, and cross-section view, respectively, of an another embodiment of a combination hole;

FIGS. 6A-6C show a perspective view, top view, and cross-section view, respectively, of an another embodiment of a hole for receiving a fastener;

FIGS. 7A-7C show a perspective view, top view, and cross-section view, respectively, of an another embodiment of a combination hole;

FIGS. 8A-8C show a perspective view, top view, and cross-section view, respectively, of an another embodiment of separate locking and non-locking holes;

FIGS. 9A-9D show a perspective view, a top view, a cross-section view, and a perspective view with a locking fastener, respectively, according to another embodiment of a plate including three overlapping locking and non-locking holes;

FIGS. 10A-10B show perspective views of a plate according to another embodiment with locking and non-locking functionality;

FIGS. 11A-11E shows alternative locking screw and openings in plates according to yet another embodiment;

FIGS. 12A and 12B depict a perspective view and cross-section view of an alternative version of a plate with blocking screws;

FIGS. 13A and 13B depict a fastener according to another embodiment with self-forming threads configured to form threads in the opening of a plate;

FIGS. 14A and 14B depict an opening in a plate according to one embodiment having a windswept cut configured to receive the self-forming threads of the fastener of FIGS. 13A-13B;

FIGS. 15A and 15B depict an opening in a plate according to another embodiment having a knurled cut configured to receive the self-forming threads of the fastener of FIGS. 13A-13B;

FIGS. 16A and 16B depict an opening in a plate according to another embodiment having a polygonal cut configured to receive the self-forming threads of the fastener of FIGS. 13A-13B;

FIG. 17A depicts an alternative opening in a plate according to another embodiment;

FIG. 17B depicts another alternative opening in a plate according to yet another embodiment;

FIGS. 18A-18D depict a plate assembly according to one embodiment where a locking or non-locking fastener may be positioned at an angle or perpendicular to the plate;

FIG. 19 depicts a stabilization system according to one embodiment including a volar distal radius dia-meta bone plate;

FIG. 20 depicts a stabilization system according to one embodiment including an acute dorsal bone plate.

FIG. 21 is a cross sectional view of the dorsal bone plate of FIG. 20;

FIG. 22 depicts a stabilization system according to one embodiment including an oblique dorsal bone plate;

FIG. 23 depicts dorsal bone plates of FIGS. 20 and 22 with fixation screws;

FIG. 24 is a close up view of a portion of the dorsal bone plates of FIGS. 20 and 22;

FIG. 25 depicts a stabilization system according to one embodiment including a lateral bone plate.

FIG. 26 is a cross sectional view of the lateral bone plate of FIG. 25;

FIG. 27 depicts the lateral bone plate of FIG. 25 with fixation screws;

FIG. 28 depicts a stabilization system according to one embodiment including a bridge bone plate;

FIG. 29 depicts a stabilization system according to one embodiment including a lunate facet hook plate;

FIG. 30 depicts the lunate facet hook plate of FIG. 29 with a fixation screw;

FIG. 31 depicts the volar distal radius plate of FIG. 1 used with the lunate facet hook plate of FIG. 30;

FIGS. 32 and 33 depict a lunate facet hook plate reduction instrument; and

FIGS. 34 and 35 depict a backpack drill guide for use with at least the volar distal radius plates of FIG. 1.

DETAILED DESCRIPTION

Embodiments of the disclosure are generally directed to devices, systems, and methods for bone stabilization, especially radius stabilization. Specifically, embodiments are directed to volar distal radius stabilization systems including a bone plate configured to sit against the volar side of the radial bone. The fasteners may be configured to secure the bone plate to the radius. Still other embodiments are directed to different types of holes and fasteners configured to provide locking and/or compression to the bone.

The bone plate may be comprised of titanium, stainless steel, cobalt chrome, carbon composite, plastic or polymer—such as polyetheretherketone (PEEK), polyethylene, ultra high molecular weight polyethylene (UHMWPE), resorbable polylactic acid (PLA), polyglycolic acid (PGA), combinations or alloys of such materials or any other appropriate material that has sufficient strength to be secured to and hold bone, while also having sufficient biocompatibility to be implanted into a body. Similarly, the fasteners may be comprised of titanium, cobalt chrome, cobalt-chrome-molybdenum, stainless steel, tungsten carbide, combinations or alloys of such materials or other appropriate biocompatible materials. Although the above list of materials includes many typical materials out of which bone plates and bone fasteners are made, it should be understood that the bone plates and fasteners comprised of any appropriate material are contemplated.

The embodiments of the disclosure and the various features and advantageous details thereof are explained more fully with reference to the non-limiting embodiments and examples that are described and/or illustrated in the accompanying drawings and detailed in the following description. The features of one embodiment may be employed with other embodiments as the skilled artisan would recognize, even if not explicitly stated herein. Descriptions of well-known components and processing techniques may be omitted so as to not unnecessarily obscure the embodiments of the disclosure. The examples used herein are intended merely to facilitate an understanding of ways in which the disclosure may be practiced and to further enable those of skill in the art to practice the embodiments of the disclosure.

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Accordingly, the examples and embodiments herein should not be construed as limiting the scope of the disclosure, which is defined solely by the appended claims and applicable law. Moreover, it is noted that like reference numerals represent similar features and structures throughout the several views of the drawings.

Volar Distal Radius Plate System

Referring now to the drawing, FIGS. 1A-1J depict embodiments of a volar distal radius stabilization system **100** including a bone plate **110** configured to sit against the volar side of the radial bone and one or more bone fasteners **130** configured to be received in the bone plate **110** and secured to the radius **102**. The radius **102** or radial bone is one of the two large bones of the forearm, the other being the ulna. The radius **102** extends from the lateral side of the elbow to the thumb side of the wrist and runs parallel to the ulna, which exceeds it in length and size. Near the wrist, the distal end **104** of the radius **102** is large and of quadrilateral form. Although generally described with reference to the radius **102**, it will be appreciated that the stabilization systems described herein may be used or adapted to be used for the fixation of other long bones as well, such as the humerus, femur, tibia, etc.

The bone plate **110** extends from a first end **112** configured to be positioned proximate to a shaft portion of radius **102** to a second end **114** configured to be positioned proximate to the distal end **104** of the radius **102**. The plate **110** includes a top surface **116** and an opposite, bottom surface **118** configured to contact adjacent bone. The top and bottom surfaces **116**, **118** are connected by opposite side surfaces extending from the first to second ends **112**, **114** of the plate **110**. The bottom surface **118** of the plate **110** includes an anatomic contour configured to follow the best approximation of average distal radial anatomy, flaring up slightly along the radial column and more significantly along the intermediate column of the plate **110**. The plate **110** is designed to sit low and have a generally low profile proximal portion. The thickness of the plate **110** may generally be about 2 mm along the shaft and distal intermediate column, tapering to a thickness of 2.5 mm along the distal radial column which allows for the severe angle of the radial styloid fastener. The watershed line of the volar distal radius defines the border between the radiocarpal (RC) joint and the volar surface of the radius **102**. A chamfer at the second end **114** on the distal radius column of the plate **110** may help to ensure minimal tendon disruption, for example of the flexor pollicis longus and flexor carpi radialis, by maintaining a lower profile over the tendon sites.

The bone plate **110** includes an elongated portion **140** extending along a longitudinal axis L, having a length greater than its width. The elongated portion **140** is configured to contact the shaft of the radius **102**. The elongated portion **140** may terminate at the first end **112** with a taper such that it has a width and/or thickness less than the remainder of the elongated portion **140**. A transition region **144** may connect the elongated portion **140** to an enlarged head portion **142**. The transition region **144** may extend along an axis T which is generally angled relative to the axis L of the elongated portion **140**. The transition region **144** may extend at an angle X relative to the elongated portion **140**. The angle X of the transition region **144** relative to the elongated portion **140** may range from about 10-60°, about 20-50°, about 30-40°, about 40-50°, or another appropriate angle. The transition region **144** may generally form a curve from the elongated portion **140** to an end of the enlarged head portion **142**.

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The transition region **144** may connect to an end portion of the enlarged head portion **142** and the other end portion of the enlarged head portion **142** may be a free end. In other words, the opposite end portion of the enlarged head portion **142**, not connected to the transition region **144**, is not connected to any other portion of the plate **110**. The free end of the enlarged head portion **142** may be separated a distance from the transition region **144** and the elongated portion **140** of the plate **110**.

The enlarged head portion **142** or a portion thereof is configured to contact the distal end **104** of the radius **102**. The enlarged head portion **142** has a width greater than the width of the elongated portion **140**. The enlarged head portion **142** extends along an axis A at an angle Y relative to the transition region **144**. The angle Y of the head portion **142** relative to the transition region **144** may range from about 10-60°, about 20-50°, about 30-40°, about 40-50°, or another appropriate angle. Accordingly, the axis A of the enlarged head portion **142** may be transverse to the axis L of the elongated portion **140**. In some embodiments, the axis A of the enlarged head portion **142** may be generally perpendicular to the axis L of the elongated portion **140**. As best seen in FIG. 1C, the bone plates **110** may be available in a variety of lengths and sizes based on the anatomy of the patient. The plates **110** are configured to sit against the volar side of the radial bone **102**. The plates **110** are configured in both left and right designs, in a mirrored configuration, in order to address the anatomy of both the left and right arms of the patient.

As best seen in FIGS. 1H and 1I, the bottom surface **118** of the plate **110** may include a plurality of recesses **119** located along the elongated portion **140** between the fastener openings **120**. In the embodiment shown in FIG. 1H, the recesses **119** are in the form small partial bores in the lateral surface, which are configured to facilitate bending of the plate **110**. The recesses **119** remove material such that the plate **110** shield stress from the fastener openings **120**, discouraging hole warping effect during recontouring of the plate **110**. The recesses **119** may also provide attachment points for plate placement instrumentation (not shown). In the embodiment shown in FIG. 1I, the recesses **119** are in the form of scallop cuts having partially cylindrical valleys cut around a periphery of the bottom surface **118** of the plate **110**. This again shields stress from the fastener openings **120** during bending, discouraging hole warping effects while recontouring the plate **110**. This also reduces contact between the plate **110** and the bone surface, thereby helping to preserve blood supply to the bone and prevent osteonecrosis. In addition to or in place of the recesses **119**, a plurality of dimples, best seen in FIG. 1J, may be positioned along the bottom surface **118** of the plate **110** (e.g., along the entire bottom surface **118** or a portion thereof) to further reduce contact between the plate **110** and bone surface, further helping to preserve blood supply and prevent osteonecrosis.

The plate **110** includes one or more through openings **120** configured to receive one or more bone fasteners **130**. The openings **120** extend through the body of the plate **110** from the top surface **116** to the bottom surface **118**. The openings **120** may include cylindrical openings, conical openings, elongated openings, threaded openings, textured openings, non-threaded and/or non-textured openings, and the like. The openings **120** may allow for locking of the fastener **130** to the plate **110** or may allow for movement and dynamic compression of the bone. The plate **110** may comprise any suitable number of openings **120** in any suitable configuration. These openings **120** allow surgeons more flexibility for

fastener placement, based on preference, anatomy, and fracture location. Surgeons may have differing opinions as to the number, location, and types of fasteners **130**. Further, complexity of fracture location and shape makes having as many locations for fasteners **130** as possible necessary. This design offers surgeons a versatile method to achieve higher accuracy in placement of the fasteners **130**.

The openings **120** may be configured to receive one or more bone fasteners **130**. The fasteners **130** may include locking fasteners, non-locking fasteners, or any other fasteners known in the art. The fasteners **130** may comprise bone screws or the like. The fasteners **130** may also include other fasteners or anchors configured to be secured or engaged with bone, such as nails, spikes, staples, pegs, barbs, hooks, or the like. The fasteners **130** may include fixed and/or variable angle bone screws. The fastener **130** may include a head portion **132** and a shaft portion **134** configured to engage bone. For a locking fastener **130**, the shaft portion **134** may be threaded such that the fastener **130** may be threaded into the bone. The head portion **132** may include a textured area, such as threads, around its outer surface sized and configured to engage with the opening **120**, for example, and corresponding threads in the opening **120** in order to lock the fastener **130** to the plate **110**. In the alternative, for a non-locking fastener **130**, the head portion **132** may be substantially smooth to allow for dynamic compression of the bone.

In one embodiment, the enlarged head portion **142** of the plate **110** includes a plurality of holes **120A** are aligned so that their nominal trajectories follow the articular surfaces of both the radio-carpal joint and the distal radio ulnar-joint. This allows the fasteners **130A** to buttress and support the articular surfaces during fracture reconstruction. As shown in the embodiment in FIGS. **1A-1C**, the plate **110** may have a single row of holes **120A** generally in alignment and a secondary hole **120A** positioned on the transition region **144**. FIG. **1C** depicts one embodiment of the plate **110** (right most plate **110**) having a first, distal row of holes **120A** generally in alignment and a second row of holes **120A** generally in alignment. The second row of holes **120A** may receive fasteners **130A** with trajectories converging with the distal row screw trajectories. In an alternative version of the stabilization system **100**, shown in FIGS. **1D** and **1E**, the elongated portion **140** directly transitions into the enlarged head portion **142** and the enlarged head portion **142** is increased in dimension in order to receive the second row of the fasteners **130A**.

The holes **120A** may be fixed openings configured to accept fixed angle fasteners **130A** that can be secured into the distal end **104** of the radius **102**. The screw holes **120A** and screw heads **132** may have mating conical threads that lock the screw **130A** in both angular and axial alignment to prevent collapse and backout. The fasteners **130A** may have predetermined trajectories based on the orientations of the openings **120A**. An upper portion of the holes **120A** may be tapered **128** to allow for the proper positioning of each of the fasteners **130A**. Each of the fasteners **130A** may be angled along a different trajectory than the other respective fasteners **130A**. Some of the fasteners **130A** may have a greater angulation than other respective fasteners **130A**.

The enlarged head portion of the plate **110** further include a hole **120B** configured to receive fastener **130B** with a trajectory having the severe angle necessary to reach the tip of the radial styloid. An upper portion of the hole **120B** may be tapered **128** and a portion of the plate **110** around the hole **120B** may be enlarged or increased in thickness to allow for the proper angle of the fasteners **130B** to be achieved. The

fastener **130B** may be in the form of a polyaxial bone screw, which may be generally larger (e.g., in length and/or diameter) than the other fasteners **130** securing the plate **110** to the bone. The fasteners **130A**, **130B** are optionally cannulated to allow for precise placement with a k-wire (not shown) if desired by the surgeon. In some embodiments, the fasteners **130A**, **130B** may include polyaxial screws having self-forming threads that work by displacement of the plate material, which are described in more detail herein.

The plate **110** also include one or more holes **120C** present along the elongated portion **140** of the plate **110** and configured to accommodate a compression fastener **130C**. As best seen in FIG. **1G**, the holes **120C** may offer a sliding slot for proximal-distal adjustment of the plate **110** during provisional placement. The slot **120C** may allow for proximal adjustment, distal adjustment, and/or medial-lateral adjustment of the plate **110**. This allows surgeons to optimally center the plate position along the bone prior to locking screw insertion. The hole or holes **120C** may be elongated along the longitudinal axis **L** of the elongated portion **140** as well as elongated, relative to the fastener **130C**, from lateral side to lateral side. The elongated hole or holes **120C** may have varying lengths and/or widths. Preferably, the length is greater than the width of the slot **120C**.

The hole **120C** may be configured to accommodate non-locking, compression screws **130C**, the heads of which have a spherical underside, so the screw **130C** may be placed at varying angles. The compression screw **130C** can be inserted and preliminarily tightened to secure the plate **110** to the bone. As the screw **130C** is inserted eccentrically in to the hole **120C**, the screw **130C** slides down the slot **120C**, displacing the plate **110** and the bone as well. The compression screw **130C** may have a shorter length and/or a smaller diameter than the screws **130A** and/or **130B**. If the plate **110** needs to be adjusted later, the screw **130C** can be loosened and the plate **110** can be shifted in the proximal, distal, and/or medial-lateral directions. This slot **120C** also accommodates reduction of the radius **102** by inserting a longer compression screw **130C** and pulling the bone to the plate **110**.

The plate **110** may include one or more holes **120D** present along the elongated portion **140** of the plate **110** configured to secure the plate **110** to the shaft of the radius **102**. The holes **120D** may be configured to accommodate fixed and/or variable angle fasteners **130D**. For locking fasteners **130D**, the screw holes **120D** and screw heads **132** may have mating conical threads that lock the screw **130D** in both angular and axial alignment to prevent collapse and backout. An upper portion of the holes **120D** may be tapered **128**, for example, around the perimeter of the hole **120D**, to allow for the proper positioning of each of the fasteners **130D**. For non-locking fasteners **130D**, the head portion **132** may be substantially smooth to allow for dynamic compression of the bone.

The plate **110** including head portion **142** and/or the elongated portion **140** may further comprise a plurality of openings **124** configured to receive one or more k-wires (not shown). The k-wire holes **124** may comprise small diameter holes (e.g., having a diameter significantly smaller than the fastener openings **120**). The k-wire holes **124** may allow preliminary placement of the plate **110** against the bone and/or to aid in reduction of the fracture. The distal k-wire holes **124** on the head portion **142** may ensure a trajectory to follow the RC joint and provide direction during insertion of the distal locking screws. The proximal k-wire holes in the elongated portion **140** of the plate **110** are arranged between fastener openings **120** and may be angled relative

to the surface of the plate **110** to avoid intrusion into areas where instrumentation must pass during screw insertion.

In the embodiment shown in FIGS. **1D** and **1E**, the plate **110** may also comprise a window **126**. The window **126** may provide visualization of the plate **110** with respect to the radius **102** in the operating environment and on imaging (e.g., fluoroscopy). The window **126** is shown as generally an asymmetrical triangle, but it is envisioned that the window **126**, if present, may be of any suitable shape, size, and dimension.

The bone plate **110** may be attached to a proximal humerus to fixate one or more bone fractures or fragments and thereby promote healing of the bone. In one embodiment, the plate **110** further restores the anatomic alignment of the radius **102**. The plate **110** may be positioned against the volar side of the radial bone. One or more k-wires may be supplied through the k-wire holes **124** to assist with preliminary placement of the plate **110**. Pilot holes may be drilled through the fastener openings **120** to prepare to receive the respective fasteners **130**. The fasteners **130A**, **130B**, **130C**, **130D** may be positioned through the respective openings **120A**, **120B**, **120C**, **120D** and into the radius **102**. The fasteners **130** may be affixed to the bone in any suitable order, number, and orientation depending on the anatomy of the bone and the fracture.

Alternative Hole Configurations

The fixed and variable angle, locking and non-locking openings **120**, **220** (e.g., including openings **120A**, **120B**, **120C**, **120D**) and respective fasteners **130**, **230** (e.g., including **130A**, **130B**, **130C**, **130D**) described herein may be substituted with or include one or more of the following openings **20** and/or fasteners **30**, **40**. The openings **20** and/or fasteners **30**, **40** are generally described with reference to a generic plate **10**, which may include plate **110**, **210**, **310**, **410**, **510**, **610**, or any other suitable plate design.

Referring now to the drawing, FIGS. **2-18** depict alternative openings **20** in plate **10**. The openings **20** extending through the plate **10** are configured to accept locking fasteners **30**, non-locking fasteners **40**, or a combination of both locking and non-locking fasteners **30**, **40** that are able to dynamically compress the bone and/or affix the plate **10** to the bone. When plating diaphyseal bone, surgeons may use a combination of both locking and non-locking fasteners **30**, **40** that are able to dynamically compress bone and to connect the bone and the plate **10**. Dynamic compression may also be desirable to create interfragmental compression while tightening the fasteners **30**, **40**.

The plate **10** includes a top surface **16** and an opposite, bottom surface **18** configured to contact adjacent bone. The plate **10** includes one or more through openings **20** configured to receive one or more bone fasteners **30**, **40**. The openings **20** extend through the body of the plate **10** from the top surface **16** to the bottom surface **18**. In the embodiments depicted in FIGS. **2-3**, for example, the openings **20** may be in the form of a combination opening that has at least two overlapping holes. As shown in FIG. **2**, the combination opening **20** includes a first hole **22** overlapping a second hole **24**. One of the holes **22** may be configured to be the locking hole **22**, thereby able to receive and secure the locking fastener **30** to the plate **10**, and the other of the holes **24** may be configured to be the dynamic compression hole **24**, thereby allowing the non-locking fastener **40** to freely move in the hole **24** and apply dynamic compression. The locking hole **22** may have one or more locking features designed to engage with a locking fastener **30**, and the dynamic compression hole **24** may be elongated, for example, along the central longitudinal axis of the plate **10**. The screw holes **22**,

24 are not constrained to parallel axes. This hole geometry may be used in bone plates **10** to utilize either fixed angle or variable angle locking screws **30** and/or polyaxial non-locking screws **40** that can achieve dynamic compression.

These openings **20** allow surgeons more flexibility for fastener placement, based on preference, anatomy, and fracture location. Surgeons may have differing opinions as to whether non-locking or locking screws **30**, **40** (or some combination of the two) should be used in diaphyseal bone. Further, complexity of fracture location and shape makes having as many locations for fasteners **30**, **40** as possible necessary. This design offers surgeons a versatile method to achieve higher accuracy in placement of locking and/or non-locking screws **30**, **40**.

As best seen in FIG. **2**, the locking and non-locking fasteners **30**, **40** are shown. The locking and non-locking fasteners **30**, **40** may include traditional fasteners known in the art. The locking and non-locking fasteners **30**, **40** may comprise bone screws or the like. The fasteners **30**, **40** may also include other fasteners or anchors configured to be secured or engaged with bone, such as nails, spikes, staples, pegs, barbs, hooks, or the like. The fasteners **30**, **40** may include fixed and/or variable angle bone screws.

The locking fastener **30** may include a head portion **32** and a shaft portion **34** configured to engage bone. The shaft portion **34** may be threaded such that the fastener **30** may be threaded into the bone. The head portion **32** of the locking fastener **30** includes a textured area **36** around its outer surface sized and configured to engage with the locking hole **22** of the combination opening **20**. The textured area **36** may include threads, ridges, bumps, dimples, serrations, or other types of textured areas. As shown, the texture area **36** preferably includes a threaded portion extending substantially from the top of the head portion **32** to the bottom of the head portion **32** proximate to the shaft portion **34**. Thus, when the textured area **36** engages the locking hole **22**, the locking fastener **30** is thereby locked to the plate **10**.

The non-locking fastener **40** includes a head portion **42** and a shaft portion **44** configured to engage bone. The shaft portion **44** may be threaded such that the fastener **40** may be threaded into the bone. The head portion **42** of the non-locking fastener **40** is substantially smooth around its outer surface such that it is able to slide along the elongated compression hole **24**. Thus, the non-locking fastener **40** may be coupled to the plate **10**, but not locked thereto to enable dynamic compression of the bone. It will be recognized that the head portions **32**, **42** of the fasteners **30**, **40** may include a recess configured to receive a driver or the like.

The locking hole portion **22** of the combination opening **20** includes a textured portion **26**. The textured portion **26** may include threads, ridges, bumps, dimples, serrations, knurls, or other types of textured areas. The textured portion **26** may be of the same type (e.g., mating surfaces) or different from the textured area **36** of the locking fastener **30**. As shown, the textured portion **26** is serrated or knurled along an inner portion of the hole **22**. The knurled surface may include straight, angled, or crossed lines cut or rolled into the material. In the embodiment shown in FIG. **2**, the textured portion **26** extends along substantially the entire inner surface of the hole **22**. With reference to the embodiment shown in FIG. **3**, the combination hole **20** is substantially the same as that shown in FIG. **2** except that the textured portion **26** of the locking hole **22** now includes a thin centralized textured ribbon of material. For example, the textured portion **26** takes up about half or less of the surface area of the hole **22**. In this instance, only a portion of the

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textured area 36 of the head portion 32 of the locking fastener 30 engages with and locks to the textured portion 26 of the hole 22.

An upper portion of the hole 22 may be tapered 28, without texturing, for example, to facilitate alignment of the fastener 30 with the opening 20. As shown in FIG. 3, this tapered portion 28 is enlarged in area relative to the embodiment in FIG. 2. The hole 22 may be configured to receive a fixed or variable angle fastener 30. The hole 22 may be generally conical in shape such that it is wider near the top surface 16 of the plate 10 and narrower toward the bottom surface 18 of the plate 10. The tapered portion 28 and/or the textured area 26 may be conical in shape. In this embodiment, the locking hole 22 is a textured fixed angle conical hole configured to receive locking fastener 30. The textured holes 22 may deform as the fastener head 32 interferes with the textured portion 26 of the hole 22, thereby providing a positive lock between the fastener 30 and the plate 10.

The second hole portion 24 of the combination opening 20 may be an elongated dynamic compression hole. The dynamic compression hole 24 may be elongated such that it has a length greater than its width. The hole 24 may be elongated along the longitudinal axis of the plate 10. In the alternative, the hole 24 may be generally cylindrical such that the hole 24 only permits polyaxial movement of the fastener 40. The inner surface of the hole 24 may be substantially smooth such that the non-locking fastener 40 is able to freely pivot and/or slide along the hole 24. This provides for at least two directions of compressive force (e.g., along the longitudinal axis and perpendicular to the longitudinal axis of the plate 10). The head portion 42 of the non-locking fastener 40 may be substantially smooth around its outer surface. The head portion 42 is sized and configured to engage with and be retained within the hole portion 24 of the combination opening 20. The hole 24 may be configured to receive a fixed or variable angle fastener 40. In one embodiment, the hole 24 may be generally conical in shape and/or tapered such that it is wider near the top surface 16 of the plate 10 and narrower toward the bottom surface 18 of the plate 10. In this embodiment, the hole 24 is a smooth variable angle conical hole configured to receive the non-locking fastener 40. The hole 24 may receive the fastener head 42 allowing movement of the fastener 40, for example, in a polyaxial fashion and/or along the length of the hole 22, thereby providing dynamic compression of the bone.

Turning now to FIGS. 4-7, alternative types of openings 20A-20G, which provide for locking and/or non-locking, dynamic compression are provided. As many of the features of these openings are similar to the combination openings 20 described already for FIGS. 2-3, only the different features will be further explained.

With reference to FIGS. 4A-4C, the combination opening 20A is similar to combination opening 20 except that the dynamic compression hole 24A has the same general diameter as the locking hole 22A, and the locking hole 22A includes a different type of textured portion 26A. In this embodiment, the locking hole 22A has a first diameter D1, and the dynamic compression hole 24A has a second diameter D2. Unlike the elongated hole 24 described earlier, dynamic compression hole 24A has substantially same diameter as the locking hole 22A. Thus, the first and second diameters D1, D2 are substantially the same. The hole 24A may be formed by milling or drilling a sphere out of the plate 10 in the center of the circle with tapers or ramps on either side. The hole 24A is not elongated, but is generally circular and the non-locking fastener 40 will be allowed to translate in the hole 24A because the diameter of the head portion 42

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and/or shaft (e.g., bone thread) will be smaller than the size of the hole 24A in the plate 10. With respect to hole 22A, the textured portion 26A of the hole 22A may be in the form of a tapered thread. This tapered thread may generally correspond to a similar tapered thread on the locking fastener 30. This hole 22A also does not include a tapered portion, and the textured portion 26A begins at the intersection with the top surface 16 of the plate 10. This alternative opening 20A also provides for the use of both locking and non-locking fasteners 30, 40 that are able to dynamically compress bone and/or lock the plate 10 to the bone.

Turning now to FIGS. 5A-5C, the combination opening 20B is similar to other combination openings except that the locking hole 22B includes a different type of textured portion 26B. The textured portion 26B includes a series of alternating recesses and protrusions around a central portion of the hole 22B. The recesses may be in form of a wave of alternating cutouts extending around the inner perimeter of the hole 22B. The textured portion 26B may lock the fastener 30 with a friction fit or may be modified during insertion of the fastener 30 to form a lock in situ. In this embodiment, the locking hole may allow for polyaxial locking. The plate 10 and the locking fastener 30 may be made of dissimilar materials having dissimilar hardness values. For example, the fastener 30 may have a higher hardness (e.g., on the Rockwell scale) relative to the plate 10, which may be formed of a material having a lower relative hardness value. Due to the increased hardness, the head portion 32 of the locking fastener 30 may create a thread in the plate 10 as the fastener 30 is inserted (e.g., threaded) into the hole 22B, thereby locking the fastener 30 to the plate 10.

With reference to FIGS. 6A-6C, the opening 20C includes locking hole 22C and dynamic compression hole 24C with a more open configuration. The locking portion 22C has a textured portion 26C in the form of a tapered thread. This tapered thread may generally correspond to a similar tapered thread on the locking fastener 30. The opposite portion 24C of the opening 20C is oblong with a ramp 25C milled into the top surface 16 of the plate 10 to allow for dynamic compression. As best seen in FIG. 6C, the ramp may be partially spherical in shape and extend from the top surface 16 of the plate 10 and connect to the textured portion 26C. When viewed from above in FIG. 6B, the ramp 25C creates a square-like, key-hole, and/or non-hole geometry that sweeps into the tapered threaded locking hole 22C. This alternative opening 20C also provides for the use of both locking and non-locking fasteners 30, 40 that are able to dynamically compress bone and/or lock the plate 10 to the bone.

Turning now to FIGS. 7A-7C, the opening 20D includes locking hole 22D and dynamic compression hole 24D. These holes 22D, 24D are connected and close together but are not overlapping. The holes 22D, 24D are separated by a small portion or sliver of plate material proximate to the lower portion of the holes 22D, 24D (e.g., at bottom surface 18 of the plate 10 and partially extending between the holes 22D, 24D). The locking portion 22D has a textured portion 26D in the form of a tapered thread. The textured portion 26D extends around almost the entire circumference of the hole 22D except where connected to hole 24D. The dynamic compression hole 24D is elongated and has ramped portions 25D on opposite sides of the hole 24D to receive fastener 40. This configuration allows for a very close population of holes 22D, 24D on the plate 10 while giving structural stability at the holes 22D, 24D.

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With reference to FIGS. 8A-8C, locking hole 22E and dynamic compression hole 24E are adjacent, but separate from one another. The holes 22E, 24E are completely separated from one another by a wall 56 of plate material. The locking portion 22E has a textured portion 26E in the form of a tapered thread extends around the entire perimeter of the hole 22E. The dynamic compression hole 24E is elongated and has ramped portions 25E on opposite sides of the hole 24E. This configuration also allows for a very close population of holes 22E, 24E on the plate 10 while giving options for both locking and/or dynamic compression.

Turning now to FIGS. 9A-9D, an alternative version of opening 20F is provided. In this embodiment, the hole construct 20F is comprised of at least three overlapping conical threaded holes in the plate 10. The opening 20F includes a first, locking hole 22F, a second hole 24F, and a third hole 23F arranged along a longitudinal axis of the plate 10. The third hole 23F is the mirror image of hole 24F across the first locking hole 22F. The conically threaded holes 22F, 23F, 24F may or may not have parallel axes. Each hole 22F, 23F, 24F may include a textured portion 26F, for example, in the form of one or more threaded portions. Thus, the locking fastener 30 may lock to any of the holes 22F, 23F, 24F. Although each of the holes 22F, 23F, 24F are shown in with the textured portion 26F, it will be appreciated that one or more of the holes 22F, 23F, 24F may have a substantially smooth inner portion instead of the textured portion 26F. The upper part of the hole construct at the first and second ends of the hole 20F each have a ramped feature 25F (e.g., adjacent to holes 23F and 24F) to allow for dynamic compression of the plate 10. In addition, the ramped feature 25F may span the three or more conical holes 22F, 23F, 24F (e.g., around the entire perimeter of the opening 20F).

The non-locking compression fasteners 40 may have a major bone thread diameter such that the fastener 40 can translate between overlapping holes 22F, 24F, 23F without interference. As best seen in FIG. 9D, the locking fastener 30 may include a textured area 36, for example, in the form of a thread, configured to engage with the textured portion 26F of any of the holes 22F, 23F, 24F. The hole geometry of opening 20F can be applied to bone plates 10 to utilize either fixed angle and/or variable angle locking screws 30 and/or polyaxial non-locking screws 40 that can achieve dynamic compression. This allows surgeons more flexibility for screw placement, based on preference, anatomy, and fracture location.

Turning now to FIGS. 10A-10B, another embodiment of opening 20G is provided. This opening 20G may be comprised of one elongate hole or slot extending from the top surface 16 to the bottom surface 18 of the plate 10. A locking portion 22G of the opening 20G may include a textured portion 26G having straight machine threads. The threads may extend more than 180 degrees to retain the locking fastener 30. A non-locking portion 24G of the opening 20G may be positioned opposite the locking portion 22G to complete the opening 20G. The upper part of the opening 20G may have one or more ramped features 25G to allow for dynamic compression of the plate 10. The ramp 25G may span along the entire upper perimeter of the elongated slot 20G or a portion thereof. The compression screws 40 may have a major bone thread diameter such that the screws 40 are able to translate along the opening 20G without interference.

With reference to FIGS. 11A-11E, alternative embodiments of the locking fastener 30 may be used with any plate 10. The head portion 32 of the fastener 30 may include a textured area 36 in the form of a thread, for example, to lock

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the fastener 30 to the plate 10. The fastener 30 and/or plate 10 may also include one or more mechanisms to prevent back out of the fastener 30 from the plate 10. In FIG. 11A, the head portion 32 includes a threaded portion 36A (e.g., having straight threads) that interface with the plate 10 and the top of the head extends larger than the threads. The head portion 32 bottoms out when the fastener 30 is fully inserted and creates preload in the fastener 30, thus locking the fastener 30 rotationally. In FIG. 11B, the head portion 32 includes threaded portion 36B. The head portion 32 has a constant major diameter while the minor diameter is tapered. The thread depth may go to zero at the top of the head portion 32 of the screw 30. The first few turns smoothly insert, but as the tapered portion of the male thread engages with the plate 10, interference occurs, jamming and/or locking the screw 30 and preventing backout. In FIG. 11C, a screw thread 36C on the head portion 32, similar to the design in FIG. 11B, except the minor diameter of the screw 30 stays constant while the major diameter of the head portion 32 gets larger toward the top of the screw 30. A similar jamming and locking mechanism results through tightening of the screw 30 in the plate 10. In FIG. 11D, the threaded portion 36D has areas of varying pitch. In particular, a straight screw thread on the head portion 32 of the screw 30 has a similar pitch to that of the plate 10 at the bottom of the head portion 32 of the screw 30. The pitch then increases or decreases towards the top of the head portion 32, which thereby results in jamming of the threads and preventing unwanted backout of the screw 30. In an alternative variation of the concept of FIG. 11D, shown in FIG. 11E, the opening in the plate 10 is provided with areas of varying pitch while the pitch of the threaded portion 36D remains constant. For example, the head portion 32 may include a straight thread with a constant pitch. The upper surface of the plate 10 may include a thread pitch is similar to that of the screw 10, but towards the bottom surface of the plate 10, the thread pitch would either increase or decrease to lock the screw 30 to the plate 10.

Turning now to FIGS. 12A and 12B, the plate 10 includes an additional anti-backout feature. In this embodiment, the plate 10 includes cylindrical holes or openings 20H configured to accept either the compression fastener 40 or the locking fastener 30. Each opening 20H may include a ramped portion 25H extending around a portion or the entire perimeter of the opening 20H to allow for dynamic compression with a compression fastener 40. Each opening 20H may include a cylindrical feature to provide angular stability with a locking fastener 30. The opening 20H may also include an angular taper 28 to cause compressive tightening between the locking fastener 30 and the cylindrical opening 20H. Each opening 20H has an accompanying blocking screw 46 that can be actuated to block the fastener 30, 40 from backing out. The blocking screw 46 may extend from a first end at the top surface 16 to a second end at the bottom surface 18 of the plate 10. The first end of the blocking screw 46 may include a recess sized to receive an instrument to rotate the blocking screw 46 from an unblocked position to a blocked position. The blocked position may include a portion of the blocking screw 46 covering a portion of the head portion 42 of the fastener 40, thereby further preventing backout of the fastener 40 from the plate 10.

According to yet another embodiment, the plate 10 may include one or more openings 20 configured to receive the locking fastener 30 having self-forming threads that work by displacement of the plate material to lock the fastener 30 to the plate 10. Turning now to FIGS. 13-18, the locking fastener 30 and alternative embodiments of the openings 20

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in the plate **10** are shown. In these embodiments, the locking mechanism of the fastener **30** (e.g., bone screw) to the internal fixation plate **10** may allow for variable angle screw insertion. The fastener **30** may be inserted within an angular cone where the force required to dislodge the head portion **32** of the fastener **30** is substantially equivalent to the force required when the fastener **30** is inserted perpendicular to the plate **10**. The holes or openings **20** in the plate **10** may be shaped such that the fastener **30** may be inserted at different angles. The geometry of the opening **20** is conducive to catching the threads on the head portion **32** of the fastener **30** and to reduce the axial force necessary to initiate the thread formation.

The locking mechanism includes a fastener **30** having a head portion **32** with self-forming threads that displace the plate material. The plate **10** may be made of a material softer than the fastener **30** to facilitate displacement. For example, the plate **10** may be comprised of titanium, alloys, polymers, or other materials having a lower material hardness (e.g., Rockwell hardness). The fastener **30** may be made of a harder relative material, for example, comprised of cobalt chrome, tungsten, alloys, or other materials having a higher material hardness. Preferably, the fastener **30** is comprised of a material having a strong, stiff, and high surface hardness which facilitates the thread forming process. The forming mechanism works by displacement of material rather than removal of the material of the plate **10**, thereby minimizing fragments or chips which are created from tapping.

In FIGS. **13A-13B**, the locking fastener **30** includes a head portion **32** and a shaft portion **34** configured to engage bone. Although not shown, the shaft portion **34** may be threaded such that the fastener **30** may be threaded into the bone. The head portion **32** may be tapered (e.g., at an angle of about 20°) such that the fit within the opening **20** in the plate **10** becomes tighter as the fastener **30** is advanced into the bone. The head portion **32** of the locking fastener **30** includes a textured area **36** around its outer surface sized and configured to engage an opening **20** in the plate **10**. The textured area **36** may include threads, ridges, bumps, dimples, serrations, or other types of textured areas. As shown, the textured area **36** preferably includes a threaded portion extending substantially from the top of the head portion **32** to the bottom of the head portion **32** proximate to the shaft portion **34**. The threads **36** may run generally perpendicular to the conical surface of the head portion **32**. The threaded portion **36** is in the form of self-forming threads configured to displace the plate material and create threads in the opening **20** of the plate **10**. The threaded portion has an exaggerated sharp thread peak to facilitate cutting or forming of the plate material.

Turning now to FIGS. **14-17**, alternative versions of the openings **20** are shown before being tapped with the fastener **30**. Once the fastener **30** is inserted, these openings **20** are modified based on the self-forming threads. The geometry of the openings **20** are conducive to catching the threads **36** and designed to reduce the axial force necessary to initiate the thread formation. An upper portion of the hole **20** may be tapered **28**, for example, with a conical straight tapered surface cut through the top surface **16** of the plate **10** for clearance of the head portion **32** of the fastener **30** during off angle insertion. A lower portion of hole **20** may further be tapered **29**, for example, with a conical straight tapered surface cut through the bottom surface **18** of the plate **10** for clearance of the shaft portion **34** during off angle insertion. The upper tapered portion **28** may be larger, for example, with a larger degree of taper than the lower tapered portion **29**. For example, the upper tapered portion **28** may have a

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taper in a range from about $60-90^\circ$, $70-80^\circ$, or $72-78^\circ$, preferably about 70° , 75° , or 80° whereas the lower tapered portion **29** may have a taper in a range from about $50-70^\circ$, $55-65^\circ$, or $57-63^\circ$, preferably about 55° , 60° , or 65° . The upper and/or lowered tapered portions **28**, **29** may be substantially conical (e.g., FIGS. **14B**, **15B**, **16B**) or may be segmented with more than one section, such as two separate conical sections having different diameters or degrees of taper (e.g., FIGS. **17A** and **17B**).

At the intersection between the upper tapered portion **28** and the lower tapered portion **29** a narrowed central portion may have a textured portion **26**. As described herein, the textured portion **26** may include threads, ridges, bumps, dimples, serrations, or other types of textured areas. In the embodiment shown in FIGS. **14A-14B**, the textured portion **26** includes a windswept cut design comprised of a plurality of shallow cuts where each cut overlaps the next. For example, the windswept design may include a plurality of threadlike helical cut sweeps. Each cut has a smooth transition into the inner diameter of the hole **20** (e.g., into the upper and lower tapered portions **28**, **29**). The windswept cuts provide a positive surface for the self-forming threads to cut into, thereby helping to prevent peeling of the newly formed threads into the plate **10**.

In FIGS. **15A-15B**, the textured portion **26** includes a knurled cut design. A rounded transition between the upper tapered portion **28** and the lower tapered portion **29** (e.g., the two conical cuts) provides a workable surface for the knurling process as well as a surface for the head portion **32** to be able to roll over during off-axis locking. The knurled design may include a plurality of shallow knurled grooves set in a diamond pattern (e.g., about 45°) where each cut overlaps the next. The knurled grooves allow for the self-forming threads to cut more deeply into the material and reduce the necessary axial force to begin the thread forming process. FIGS. **16A-16B** depict a polygon form cut design. In this design, there is no textured portion at the transition between the upper tapered portion **28** and the lower tapered portion **29**. Instead, the narrowed central region has an overall polygonal form such that the hole **20** is neither cylindrical nor conical. The polygonal shape includes a number of sides with distinct linear section of material and rounded corners around which the form cut is allowed to sweep. For example, the polygonal shape may be substantially hexagonal (6-sided), heptagonal (7-sided), octagonal (8-sided), etc. The hole **20** may also be represented without lobe cuts, as a single concentric ring with the same geometry.

In FIG. **17A**, the upper tapered portion **28** includes a conical straight tapered surface cut for clearance of the head portion **32** of the fastener **30** during off angle insertion. The upper tapered portion **28** is segmented to have an upper area with a larger area relative to a lower area proximate the transition to the lower tapered portion **29** having a narrower diameter. The central area between the upper and lower tapered portions **28**, **29**, where the thread forming process occurs, includes two peaks or concentric rings of material (e.g., a superficial ring **60** and a deep ring **62**) with a groove **27** being located in between for material removal and thread forming relief. The groove **27** between the rings **60**, **62** may be angled, for example, in the range of about $40-80^\circ$, about $50-70^\circ$, or about 60° . The superficial ring **60** is of a slightly smaller inner diameter than the deep ring **62**, as the superficial ring **60** is responsible for supporting a majority of the cantilever loads. The deep ring **62** provides additional fixation and support during off-angle insertion as well as additional support during nominal trajectory insertion. The

lower tapered portion **29** includes a straight tapered surface that provides clearance for the shaft **34** of the fastener **30** when inserted off angle.

The embodiment of the opening **20** in FIG. 17B is similar to FIG. 17A, but further includes textured portion **26** in the form of a plurality of helical swept cuts at the transition between the upper tapered portion **28** and the lower tapered portion **29**. The shallow helical cuts or windswept cuts may include a series of cuts at a steep pitch. The windswept cuts may be angled, for example, at about 50-70°, or about 60°. The same number of cuts may be made in both a clockwise and counter-clockwise fashion. The cuts may create plateaus of material protruding into the opening **20**. The resultant geometry provides positive surfaces for the fastener **30** to cut into, which can dramatically reduce the axial force necessary to lock the fastener **30** to the plate **10**. Thus mechanism does not need to rely on bone purchase in order to engage the threads in the head portion **32** of the fastener **30**. The material removed during insertion of the fastener **30** allows the self-forming threads to cut deeper by removing material which much be formed and reducing friction between the fastener **30** and the plate **10** during the forming process.

FIGS. 18A-18D depict a screw-plate assembly. The assembly, in FIG. 18C, shows the locking fastener **30** placed at an angle, other than perpendicular, to the upper surface **16** of the plate **10**. In FIG. 18D, a non-locking fastener **40** is placed generally perpendicular to the plate **10**. It will be appreciated that the locking fastener **30** and non-locking fastener **40** may be oriented at any appropriate angle relative to the plate **10**. The section view in FIG. 18C shows the thread engagement with the plate **10** in which material of the plate **10** is displaced around the threads of the fastener **30**. By using the self-forming threads, the fastener **30** is able to be inserted into the plate **10** at variable angles and engages with the plate **10** with one-step locking requiring no additional steps to lock the fastener **30** to the plate **10**. The section view in FIG. 18D show the compressive, non-locking screw **40** received in the opening **20**, without threadedly locking thereto. The non-locking screw **40** may provide for dynamic compression of the bone. Accordingly, the fasteners and openings described herein provide a wide variety of options for the surgeon, thereby providing appropriate locking and/or unlocking capability for dynamic compression depending on the desired treatment of the fracture and the bone.

Dia-Meta Volar Distal Radius Plate System

FIG. 19 depicts embodiments of a dia-meta volar distal radius stabilization system **200** including a bone plate **210** configured to sit against the volar side of the radial bone and one or more bone fasteners are configured to be received in the bone plate **210** and secured to the radius and radial shaft of a bone. Although generally described with reference to the radius and radial shaft, it will be appreciated that the stabilization system **200** described herein may be used or adapted to be used for the fixation of other long bones as well, such as the humerus, femur, tibia, etc.

The bone plate **210** extends from a first end **212** configured to be positioned on a shaft portion of radial bone to a second end **214** configured to be positioned proximate to the distal end of the radius. The plate **210** includes a top surface **216** and an opposite, bottom surface **218** configured to contact adjacent bone. The top and bottom surfaces **216**, **218** are connected by opposite side surfaces extending from the first to second ends **212**, **214** of the plate **210**. The bottom surface **218** of the plate **210** includes an anatomic contour configured to follow the best approximation of average

distal radial anatomy, flaring up slightly along the radial column and more significantly along the intermediate column of the plate **210**. The plate **210** is designed to sit low and have a generally low profile proximal portion. The thickness of the plate **210** may generally be about 2 mm along the shaft and distal intermediate column, tapering to a thickness of 2.5 mm along the distal radial column which allows for the severe angle of the radial styloid fastener. The thickness of the plate **210** may generally increase towards the first end **212** when compared to the second end **214**. In addition, the width of the plate **210** proximate the first end **212** and along the elongate portion **240** may be thicker than the width of the plate at the second end **214**. The design of plate **210** allows for an easy transition from the second end **214** of the plate **210** to the elongate portion **240** to the first end **212** of the plate **210** to address fractures proximal to the second end of the plate **214** while also providing adequate support in the radial shat of the bone.

The second end **214** of the bone plate **210** toward the elongate portion **240** of the bone plate **210** is very similar to the bone plate **110**, thus the features and disclosures set forth above relating to the bone plate **110** are equally applicable to bone plate **210** and are incorporated in their entirety herein.

Looking at the elongate portion or dia-meta portion **240** of the plate **210**, the plate **210** includes one or more through openings **220** configured to receive one or more bone fasteners. The openings **220** extend through the body of the plate **210** from the top surface **216** to the bottom surface **218**. The openings **220** may include cylindrical openings, conical openings, elongated openings, threaded openings, textured openings, non-threaded and/or non-textured openings, and the like. The openings **220** may allow for locking of the fastener to the plate **210** or may allow for movement and dynamic compression of the bone. The plate **210** may comprise any suitable number of openings **220** in any suitable configuration. These openings **220** allow surgeons more flexibility for fastener placement, based on preference, anatomy, and fracture location. Surgeons may have differing opinions as to the number, location, and types of fasteners. Further, complexity of fracture location and shape makes having as many locations for fasteners as possible necessary. This design offers surgeons a versatile method to achieve higher accuracy in placement of the fasteners.

The openings **220** may be configured to receive one or more bone fasteners. The fasteners may include locking fasteners, non-locking fasteners, or any other fasteners known in the art. The fasteners may comprise bone screws or the like. The fasteners may also include other fasteners or anchors configured to be secured or engaged with bone, such as nails, spikes, staples, pegs, barbs, hooks, or the like. The fasteners may include fixed and/or variable angle bone screws. The fastener may include a head portion and a shaft portion configured to engage bone. For a locking fastener, the shaft portion may be threaded such that the fastener may be threaded into the bone. The head portion may include a textured area, such as threads, around its outer surface sized and configured to engage with the opening **220**, for example, and corresponding threads in the opening **220** in order to lock the fastener to the plate **210**. In the alternative, for a non-locking fastener, the head portion may be substantially smooth to allow for dynamic compression of the bone.

The plate **210** may further comprise a plurality of openings **224** configured to receive one or more k-wires (not shown). The k-wire holes **224** may comprise small diameter holes (e.g., having a diameter significantly smaller than the fastener openings **220**). The k-wire holes **224** may allow

preliminary placement of the plate **210** against the bone and/or to aid in reduction of the fracture. The distal k-wire holes **224** on the head portion **242** may ensure a trajectory to follow the RC joint and provide direction during insertion of the distal locking screws. The proximal k-wire holes in the elongated portion **240** of the plate **210** are arranged between fastener openings **220** and may be angled relative to the surface of the plate **210** to avoid intrusion into areas where instrumentation must pass during screw insertion.

Dorsal Plate System

FIGS. **20-24** depict embodiments of a dorsal stabilization system **300** including bone plates **310, 410** which are configured to sit against the dorsal portion of bone. One or more bone fasteners **320C** are configured to be received in the bone plates **310, 410** to secure the plates **310, 410** to the dorsal portion of a bone. Although generally described with reference to the dorsal portion of bone, it will be appreciated that the stabilization system **300** described herein may be used or adapted to be used for the fixation of other bones as well, such as other portions of the identified bones. It should be noted that the same reference numerals are being used for plates **310, 410** because the plates are similar except for their respective first ends **312** which show different opening **320** configurations. FIG. **20** shows an acute configuration and FIG. **22** shows an oblique configuration.

As shown in FIGS. **20-22**, the plates **310, 410** each have a body that extends from a first end **312** to a second end **314**. The plates **310, 410** each include a top surface **316** and an opposite, bottom surface **318** configured to contact adjacent bone. The top and bottom surfaces **316, 318** are connected by opposite side surfaces extending from the first to second ends **312, 314** of the plate **310**. Although the plate **310, 410** are shown having a generally longitudinal body, it will be appreciated that any suitable shape and contouring of the plates may be provided depending on the location and type of fracture to be plated.

The bone plates **310, 410** include one or more openings **320**. The openings **320** extend through the plate **310, 410** from the upper surface **316** to the bottom surface **318** and are configured to accept locking fasteners and non-locking fasteners **320C**. When using the plates **310, 410** with bone, surgeons may use only locking, only non-locking or a combination of both locking and non-locking fasteners to connect the bone and the plates **310, 410**. The openings **320** may be in the form of any of the openings discussed above with respect to the volar distal radial plate system, the dia-meta plate system, and the alternative hole configurations.

The plates **310, 410** also include one or more slots **320C** present along the elongated portion **340** of the plates **310, 410** and configured to accommodate a sliding fastener **322C**, shown in FIGS. **23** and **24**. As best seen in FIGS. **20-24**, the slot **320C** may offer a sliding slot for proximal-distal adjustment of the plates **310, 410** during provisional placement. The slot **320C** may allow for proximal adjustment, distal adjustment, and/or medial-lateral adjustment of the plates **310, 410**. This allows surgeons to optimally center the plate position along the bone prior to locking screw insertion. The slot **320C** may be elongated along a longitudinal axis of the elongated portion **340** as well as elongated, perpendicular to the longitudinal axis, from lateral side to lateral side. The elongated slot **320C** may have varying lengths and/or widths. Preferably, the length is greater than the width of the slot **320C**. The plates **310, 410** may include etch lines adjacent to slot **320C** for more accurate adjustment of the plate **310** when being positioned on bone.

As best seen in FIGS. **20** and **22**, plates **310, 410** also may include a plurality of side relief cuts or scalloped edging **322** along the length of the plates **310, 410** which allows the plates **310, 410** to be bent, for example, in three dimensions.

The side relief cuts or scalloped edges **322** may be in the form of one or more curves having a widened portion along the sides of the plates **310, 410** and a narrowed portion towards the center of the plates **310, 410**. The side relief cuts or scalloped edges **322** may be positioned between consecutive openings **320**. The plurality of relief cuts or scalloped edges **322** may form a scalloped or wavy profile along the side edges of the plates **310, 410**. As a result, the plates **310, 410** are able to be shaped to a multi-contour surface without warping the openings **320**.

The plates **310, 410** may further comprise a plurality of openings **324** configured to receive one or more k-wires (not shown). The k-wire holes **324** may comprise small diameter holes (e.g., having a diameter significantly smaller than the fastener openings **320**). The k-wire holes **324** may allow preliminary placement of the plates **310, 410** against the bone and/or to aid in reduction of the fracture.

Lateral Plate

FIGS. **25-27** depict embodiments of a lateral stabilization system **500** including bone plate **510** which is configured to sit against the lateral portion of bone to address fractures on the side of the radius. One or more bone fasteners **520C** are configured to be received in the bone plate **510** to secure the plate **510** to the lateral portion of a radius of a bone. Although generally described with reference to the lateral portion of the radius of the bone, it will be appreciated that the stabilization system **500** described herein may be used or adapted to be used for the fixation of other bones, such as long bones, as well as other portions of the identified bones.

The plate **510** has a body that extends from a first end **512** to a second end **514**. The plate **510** includes a top surface **516** and an opposite, bottom surface **518** configured to contact adjacent bone. The top and bottom surfaces **516, 518** are connected by opposite side surfaces extending from the first to second ends **512, 514** of the plate **510**. Although the plate **510** is shown having a generally longitudinal body, that contours or radius upwardly to accommodate distal radius bony anatomy, it will be appreciated that any suitable shape and contouring of the plates may be provided depending on the location and type of fracture to be plated.

The bone plate **510** includes one or more openings **520**. The openings **520** extend through the plate **510** from the upper surface **516** to the bottom surface **518** and are configured to accept locking fasteners and non-locking fasteners **520C**. When using the plate **510** with bone, surgeons may use only locking, only non-locking or a combination of both locking and non-locking fasteners to connect the bone and the plate **510**. The openings **520** may be in the form of any of the openings discussed above with respect to the volar distal radial plate system, the dia-meta plate system, the dorsal plates and the alternative hole configurations.

The plate **510** also includes one or more slots **520C** present along the elongated portion **540** of the plate **510** and configured to accommodate a sliding fastener **522C**, shown in FIG. **27**. As best seen in FIGS. **25-26**, the slot **520C** may offer a sliding slot for proximal-distal adjustment of the plate **510** during provisional placement. The slot **520C** may allow for proximal adjustment, distal adjustment, and/or medial-lateral adjustment of the plate **510**. This allows surgeons to optimally center the plate position along the bone prior to locking screw insertion. The slot **520C** may be elongated along a longitudinal axis of the elongated portion **540** as well as elongated, perpendicular to the longitudinal axis, from

lateral side to lateral side. The elongated slot **520C** may have varying lengths and/or widths. Preferably, the length is greater than the width of the slot **520C**. The plate **510** may include etch lines adjacent to slot **520C** for more accurate adjustment of the plate **510** when being positioned on bone.

As best seen in FIGS. **25** and **27**, plate **510** also may include a plurality of side relief cuts or scalloped edging **522** along a portion of the length of the plate **510** which allows that portion of the plate **510** to be bent, for example, in three dimensions. The side relief cuts or scalloped edges **522** may be in the form of one or more curves having a widened portion along the sides of the plate **510** and a narrowed portion towards the center of the plate **510**. The side relief cuts or scalloped edges **522** may be positioned between consecutive openings **520**. The plurality of relief cuts or scalloped edges **522** may form a scalloped or wavy profile along the side edges of the plate **510**. As a result, a portion of the plate **510** is able to be shaped to a multi-contour surface without warping the openings **520**.

The plate **510** may further comprise a plurality of openings **524** configured to receive one or more k-wires (not shown). The k-wire holes **524** may comprise small diameter holes (e.g., having a diameter significantly smaller than the fastener openings **520**). The k-wire holes **524** may allow preliminary placement of the plate **519** against the bone and/or to aid in reduction of the fracture.

Bridge Plate

FIG. **28** depicts an embodiment of a stabilization system **600** including bone plate **610** which acts as an internal fixator for high energy comminuted distal radius fractures. The plate **610** is placed dorsally and extends from the third or second metacarpal to approximately a third to half way down the radius. One or more bone fasteners are configured to be received in the bone plate **610** to secure the plate **610** to the desired portions of bone. Although generally described with reference to the radius and metacarpals, it will be appreciated that the stabilization system **600** described herein may be used or adapted to be used for the fixation of other bones, such as long bones, as well as other portions of the identified bones.

The plate **610** has a body that extends from a first end **612** to a second end **614**. The plate **610** includes a top surface **616** and an opposite, bottom surface **618** configured to contact adjacent bone. The top and bottom surfaces **616**, **618** are connected by opposite side surfaces extending from the first to second ends **612**, **614** of the plate **610**. Although the plate **610** is shown having a generally longitudinal body that is generally planar, it will be appreciated that any suitable shape and contouring of the plates may be provided depending on the location and type of fracture to be plated.

The bone plate **610** includes one or more openings **620**. The openings **620**, which are located proximate the first end **612** and the second end **614**, extend through the plate **610** from the upper surface **616** to the bottom surface **618** and are configured to accept locking fasteners and non-locking fasteners. When using the plate **610** with bone, surgeons may use only locking, only non-locking or a combination of both locking and non-locking fasteners to connect the bone and the plate **610**. The openings **620** may be in the form of any of the openings discussed above with respect to the volar distal radial plate system, the dia-meta plate system, the dorsal plates, the lateral plates and the alternative hole configurations.

Lunate Facet Hook Plate

FIGS. **29-31** depicts an embodiment of a stabilization system **700** including hook plate **710** which is designed for fracture patterns that involve the volar ulnar corner of the

distal radius. The plate **710** may be used as a stand-alone stabilization plate or may be used in combination with a volar distal radius plate **110**, as shown in FIG. **31**.

When the plate **710** is used alone, the hooks **712** of the plate are embedded or tapped into bone to prevent the shifting of the plate in a lateral or medial direction. It is contemplated that there may be one, two, or more hooks **712**. The plate **710** also includes an opening **720** to receive a fixation screw **714**, which may aid in further fixation of the plate **710** the bone and the fracture site.

When the plate **710** is used with the volar distal radius plate, the plate **710** is configured and dimensioned such that it can be slidably placed under a pre-positioned volar distal radius plate **110**. The opening **720** will align with an opening **120** on the volar distal radius plate **110** such that a fastener will pass through the opening **120** on the volar distal radius plate **110** and the opening **720** on the plate **710**. The opening **720** can accept a locking screw or a non-locking screw.

FIGS. **32** and **33** show a lunate facet hook plate reduction instrument **810**. The instrument is capable of being connected to any quick connect handle known in the industry, such as the AO quick-connect handle. The reduction instrument **810** utilizes a two-piece contact surface that is capable of capturing a lunate facet hook plate and releasing the hook plate when it is positioned in the desired location and orientation.

FIGS. **34** and **35** depict a drill guide **910** that can be attached to second end **114** of the volar distal radius plate **110**. The drill guide **910** may include a plurality of cannulated openings **912** which correspond to each of the respective openings **120** in the plate **110**. The drill guide **910** openings **912** may be configured in order to drill the pilot holes at the appropriate trajectories for each opening **120**, and subsequently receive the respective fasteners at the correct trajectories. The drill guide **910** may also include a plurality of k-wire openings **914** which match with the k-wire openings in the plate **110**. The drill guide **910** may be secured to the plate **110** with one or more fasteners or may be secured to the plate **110** through an integrated connection system such as a thumb screw, an interference fit, etc. The fastener may thread into the plate **110** or otherwise temporarily secure the drill guide **910** to the plate **110**. The drill guide **910** may be pre-assembled to the plate **110** or may be attached at any other suitable time before or during the surgery. The fastener may be secured, for example, in the operating room, via thumb or hexalobular fastener, to attach the drill guide **910** to the plate **110**. After the pilot holes are drilled, the drill guide **910** may then be removed and the fasteners positioned through the respective openings **120**. The drill guide **910** may be relatively slim in thickness, for example, not protruding more than 10 mm above the plate **110**, to prevent impinging on soft tissue.

Although the invention has been described in detail and with reference to specific embodiments, it will be apparent to one skilled in the art that various changes and modifications can be made without departing from the spirit and scope of the invention. Thus, it is intended that the invention covers the modifications and variations of this invention provided they come within the scope of the appended claims and their equivalents. It is expressly intended, for example, that all ranges broadly recited in this document include within their scope all narrower ranges which fall within the broader ranges. It is also intended that the components of the various devices disclosed above may be combined or modified in any suitable configuration.

What is claimed is:

1. A bone plate for stabilizing a bone, comprising:

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- an elongated portion extending along a longitudinal axis;
 an enlarged head portion extending along a second axis
 from a first end to a second end;
 a transition region connecting the elongated portion to the
 enlarged head portion, the second end of the enlarged
 head portion is a free end; and
 a plurality of through holes extending through the
 enlarged head portion, the transition region, and the
 elongated portion and configured to receive one or
 more fasteners to secure the bone plate to the bone;
 wherein the transition region is curved and connects to the
 first end of the enlarged head portion, wherein at least
 a portion of the elongated portion extends along a
 curved trajectory;
 wherein the elongated portion includes a slot for receiving
 a sliding fastener for provisional alignment of the bone
 plate, and
 wherein the longitudinal axis and the second axis are
 generally perpendicular;
 wherein a length of the slot is approximately a third of a
 length of the elongated portion.
2. The bone plate of claim 1, wherein the plurality of
 through holes includes a first plurality of fixed angle holes
 positioned in general alignment along the enlarged head
 portion, and the one or more fasteners include one or more
 fixed angle fasteners configured to be received in the fixed
 angle holes, the one or more fixed angle fasteners configured
 to be aimed at a radio-carpal joint and a distal radio-ulnar
 joint.
3. The bone plate of claim 1, wherein the plurality of
 through holes includes a polyaxial hole positioned proximate
 to the end portion of the enlarged head portion connected
 to the transition region, and the one or more fasteners
 include a polyaxial fastener configured to be received in the
 polyaxial hole, the polyaxial fastener configured to be aimed
 at a radial styloid.
4. The bone plate of claim 1, wherein the elongated slot
 allows for proximal-distal and medial-lateral adjustment of
 the plate.
5. The bone plate of claim 1, wherein the transition region
 extends at an angle relative to the longitudinal axis.
6. The bone plate of claim 1, wherein the enlarged head
 portion extends at an angle relative to the transition region.
7. The bone plate of claim 1, wherein the one or more
 fasteners include fasteners having self-forming threads on a
 head portion of the fasteners, which are configured to lock
 to at least one of the plurality of through holes on the plate.

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8. The bone plate of claim 1, wherein the plate further
 comprises a second plurality of openings configured as
 k-wire holes to receive one or more k-wires.
9. The bone plate of claim 1, wherein the plate includes
 a plurality of recesses located along the elongated portion
 between the through holes, and the plurality of recesses are
 configured to facilitate bending of the plate.
10. A bone plate configured to stabilize a radius, comprising:
 an elongated portion extending along a longitudinal
 axis,
 an enlarged head portion extending along a second axis
 from a first end to a second end, and
 a transition region connecting the elongated portion to
 the enlarged head portion;
 a plurality of fixed angle holes positioned in general
 alignment along the elongated portion and configured to
 receive a corresponding plurality of fixed angle fasteners;
 a polyaxial hole positioned proximate to the end portion
 of the enlarged head portion connected to the transition
 region, the polyaxial hole configured to receive a polyaxial
 fastener; and
 an elongated slot formed in the elongated portion and
 configured to receive a fastener to allow proximal-distal
 and medial-lateral adjustment of the bone plate,
 wherein the transition region is curved and connected
 to the first end of the enlarged head portion, the
 second end of the enlarged head portion is a free end,
 wherein at least a portion of the elongated portion
 includes scalloped edges;
 wherein a length of the elongated slot is approximately
 a third of a length of the elongated portion.
11. The bone plate of claim 10, wherein the transition
 region extends at an angle relative to the longitudinal axis.
12. The bone plate of claim 10, wherein the enlarged head
 portion extends at an angle relative to the transition region.
13. The bone plate of claim 10, wherein the plate further
 comprises a second plurality of openings configured as
 k-wire holes to receive one or more k-wires.
14. The bone plate of claim 10, wherein the plate includes
 a plurality of recesses located along the elongated portion
 between the through holes, and the plurality of recesses are
 configured to facilitate bending of the plate.

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