



US010925588B2

(12) **United States Patent**
Glimsdale

(10) **Patent No.:** **US 10,925,588 B2**
(45) **Date of Patent:** **Feb. 23, 2021**

(54) **DEVICES AND METHODS FOR OCCLUDING ABNORMAL OPENINGS IN A PATIENT'S VASCULATURE**

(71) Applicant: **St. Jude Medical, Cardiology Division, Inc.**, St. Paul, MN (US)

(72) Inventor: **Mathias C. Glimsdale**, St. Michael, MN (US)

(73) Assignee: **St. Jude Medical, Cardiology Division, Inc.**, St. Paul, MN (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 152 days.

(21) Appl. No.: **16/233,197**

(22) Filed: **Dec. 27, 2018**

(65) **Prior Publication Data**

US 2019/0133563 A1 May 9, 2019

Related U.S. Application Data

(62) Division of application No. 14/243,271, filed on Apr. 2, 2014, now Pat. No. 10,201,337, which is a division
(Continued)

(51) **Int. Cl.**
A61B 17/00 (2006.01)
A61B 17/12 (2006.01)

(52) **U.S. Cl.**
CPC **A61B 17/0057** (2013.01); **A61B 17/12109** (2013.01); **A61B 17/12122** (2013.01);
(Continued)

(58) **Field of Classification Search**
CPC A61B 17/00; A61B 17/08; A61B 17/12; A61B 17/0057; A61B 17/12109;
(Continued)

(56) **References Cited**

U.S. PATENT DOCUMENTS

5,846,261 A 12/1998 Kotula et al.
5,944,738 A 8/1999 Amplatz et al.
(Continued)

FOREIGN PATENT DOCUMENTS

CN 1672644 A 9/2005
CN 101049267 A 10/2007
(Continued)

OTHER PUBLICATIONS

International Search Report for Application No. PCT/US2012/064765, dated Feb. 4, 2013.

(Continued)

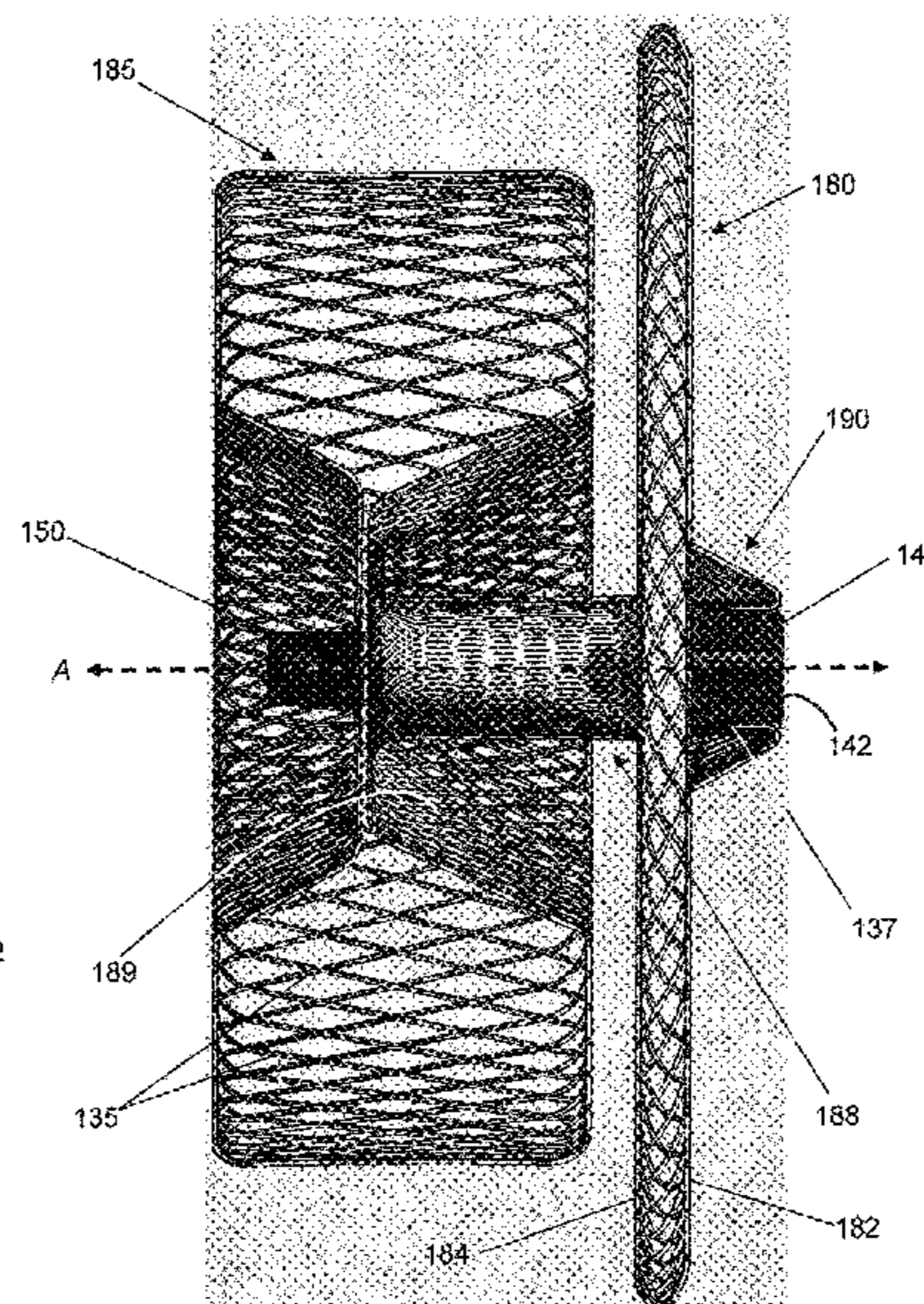
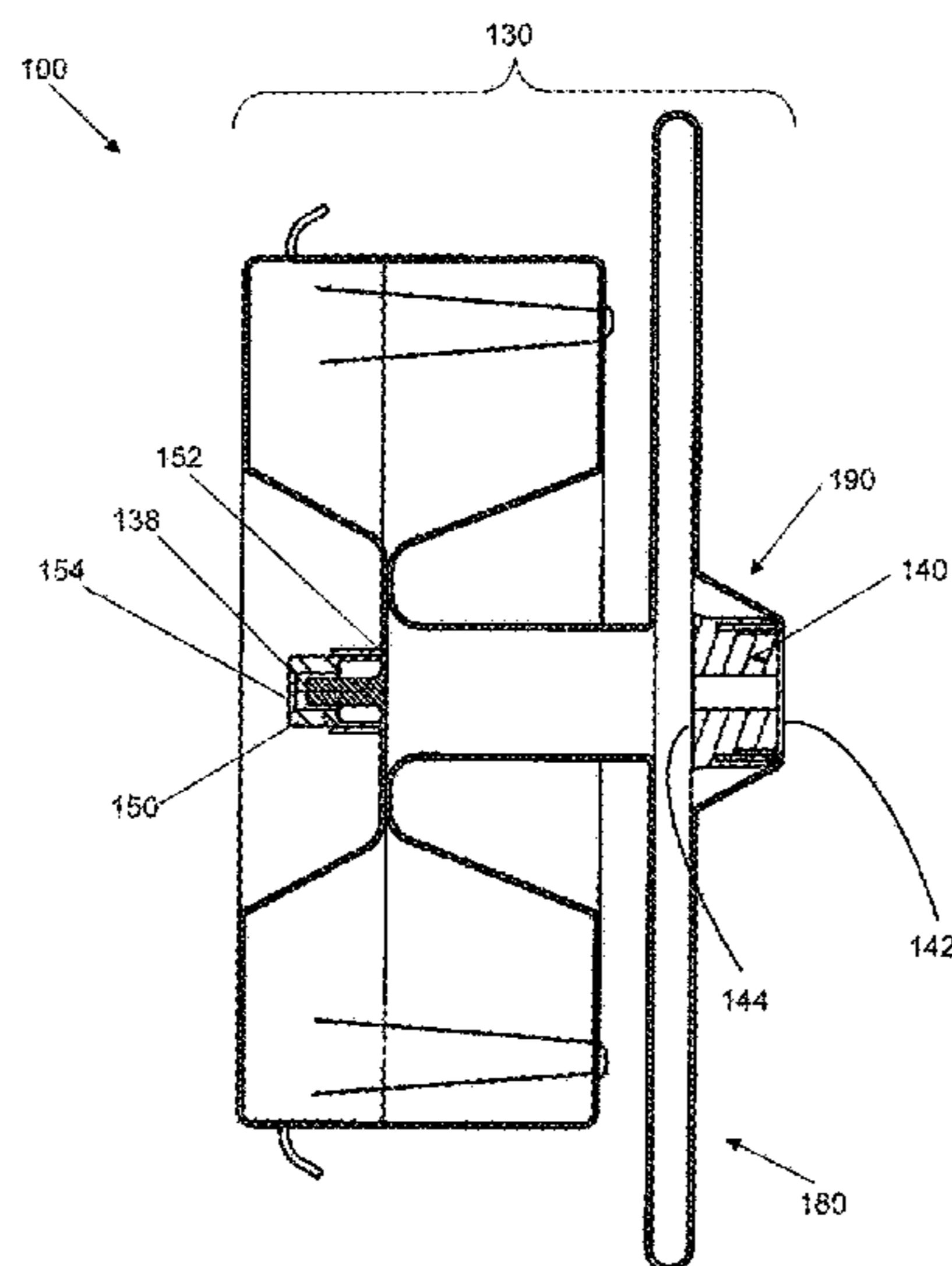
Primary Examiner — Vi X Nguyen

(74) *Attorney, Agent, or Firm* — Armstrong Teasdale LLP

(57) **ABSTRACT**

A medical device is provided in which one or both ends of the device encourage the formation of tissue across substantially the entire area of the respective end that is exposed to the blood flow for reducing the risk of a thrombotic embolism. The medical device includes a tubular structure having at least one expanded volume portion and a tapered transition portion. The tubular structure may be made through the braiding of a number of strands, and a first end feature may be used to secure the proximal strand ends. The proximal strand ends may be secured via the proximal end of the first end feature, such that the tapered transition portion is formed over the circumferential surface of the first end feature, and only a proximal end surface (or a portion of the proximal end surface) of the first end feature is exposed to the path of flowing blood.

7 Claims, 19 Drawing Sheets



Related U.S. Application Data

of application No. 13/300,322, filed on Nov. 18, 2011, now Pat. No. 8,758,389.

(52) **U.S. Cl.**

CPC .. *A61B 17/12172* (2013.01); *A61B 17/12177* (2013.01); *A61B 2017/00526* (2013.01); *A61B 2017/00579* (2013.01); *A61B 2017/00592* (2013.01); *A61B 2017/00597* (2013.01); *A61B 2017/00606* (2013.01); *A61B 2017/00623* (2013.01); *A61B 2017/00867* (2013.01); *A61B 2017/12095* (2013.01)

(58) **Field of Classification Search**

CPC *A61B 17/12122*; *A61B 2017/00637*; *A61B 2017/00654*; *A61M 29/00*
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

6,152,144	A	11/2000	Lesh et al.
6,168,622	B1	1/2001	Mazzocchi
7,862,577	B2	1/2011	Gray et al.
8,034,061	B2	10/2011	Amplatz et al.
10,201,337	B2 *	2/2019	Glimsdale <i>A61B 17/0057</i>
2001/0031981	A1	10/2001	Evans et al.
2002/0068950	A1	6/2002	Corcoran et al.
2002/0111648	A1	8/2002	Kusleika et al.

2004/0153118	A1 *	8/2004	Clubb	<i>A61F 2/013</i> <i>606/200</i>
2006/0241690	A1	10/2006	Amplatz et al.	
2007/0168019	A1	7/2007	Amplatz et al.	
2007/0233186	A1	10/2007	Meng	
2007/0265656	A1	11/2007	Amplatz et al.	
2008/0033475	A1	2/2008	Meng	
2009/0099647	A1	4/2009	Glimsdale et al.	
2009/0171386	A1	7/2009	Amplatz et al.	
2009/0306706	A1	12/2009	Osypka	
2012/0197283	A1	8/2012	Marchand et al.	

FOREIGN PATENT DOCUMENTS

CN	200970282	Y	11/2007
CN	101795628	A	8/2010
CN	102149424	A	8/2011
CN	102639181	A	8/2012
DE	102006040415	B3	1/2008
JP	2007520271	A	7/2007
JP	2008520359	A	6/2008
JP	2011005292	A	1/2011
WO	03077799	A2	9/2003
WO	2008019590	A1	2/2008
WO	2011057002	A2	5/2011

OTHER PUBLICATIONS

EP Search Report for EP Patent Application No. 19208926, dated Dec. 20, 2019, 16 pages.

* cited by examiner

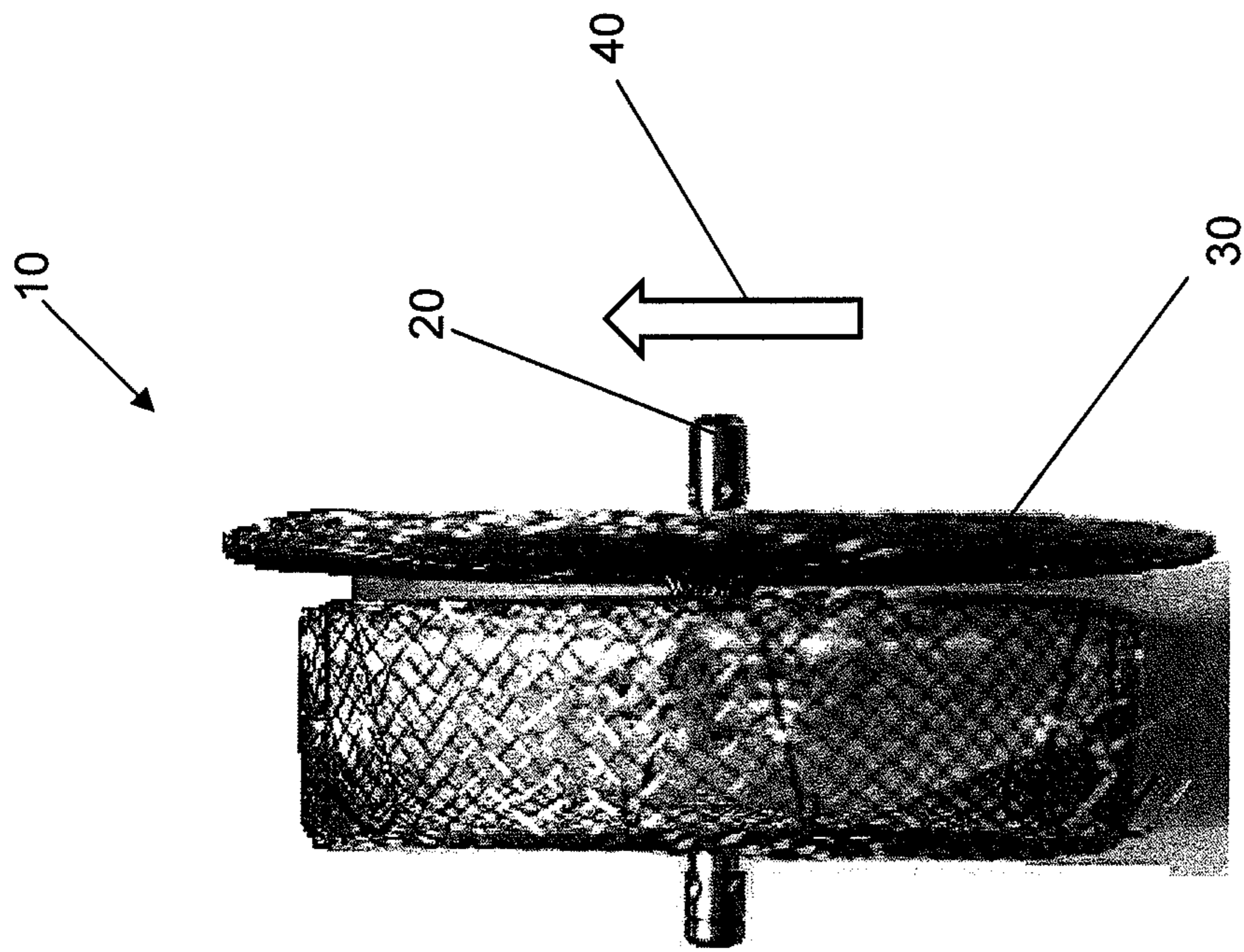


FIG. 1 (Prior Art)

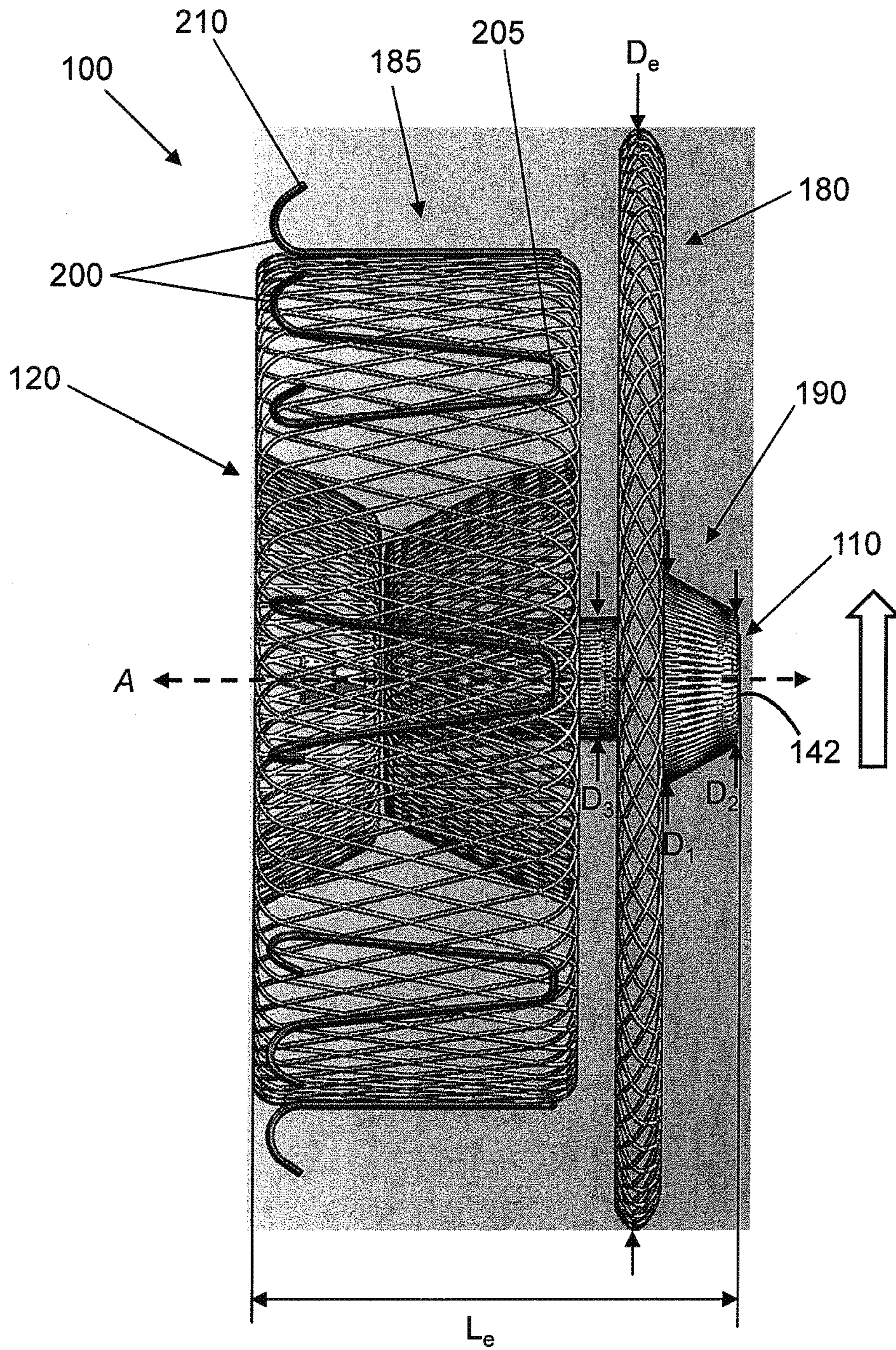


FIG. 2

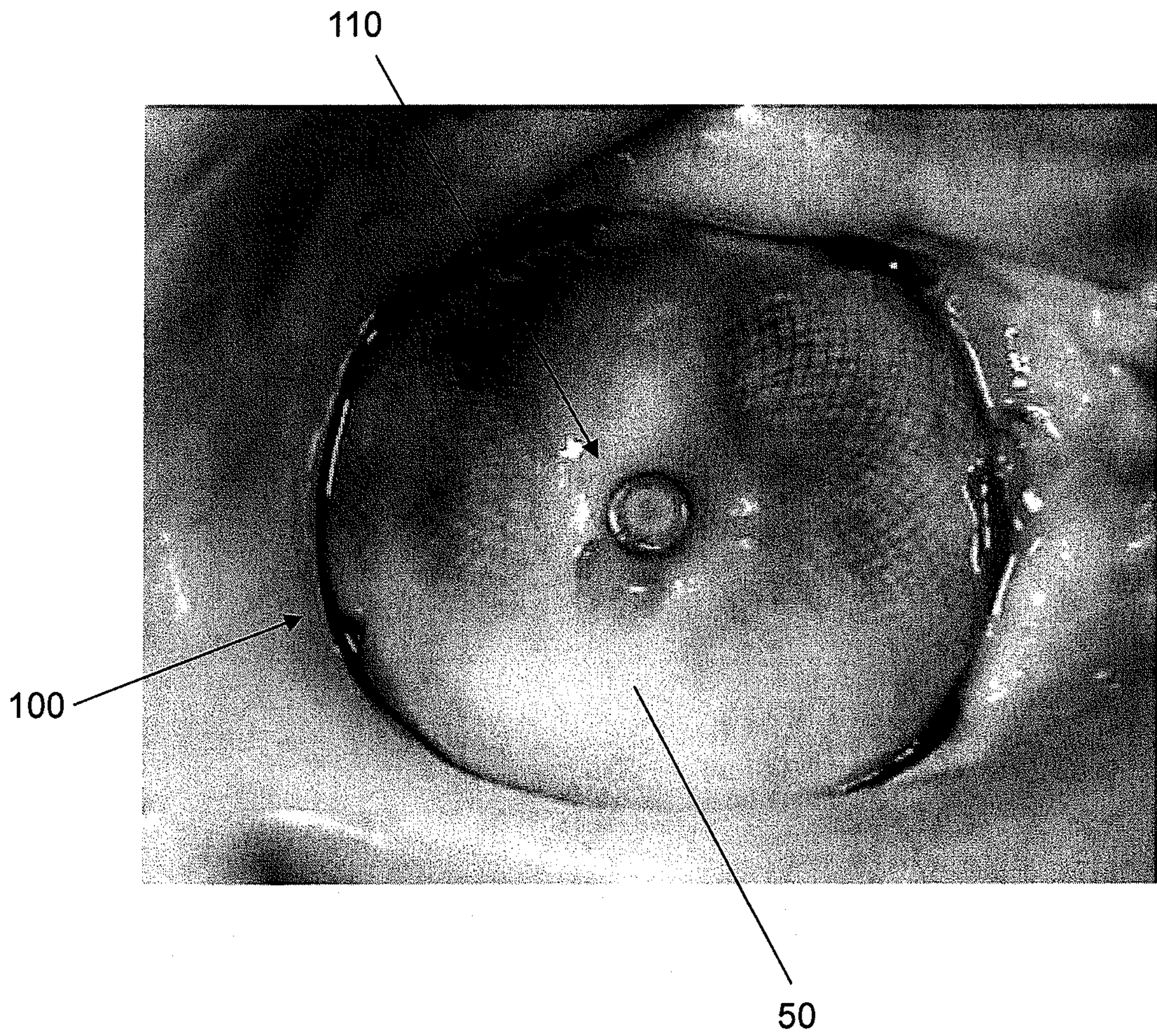


FIG. 3

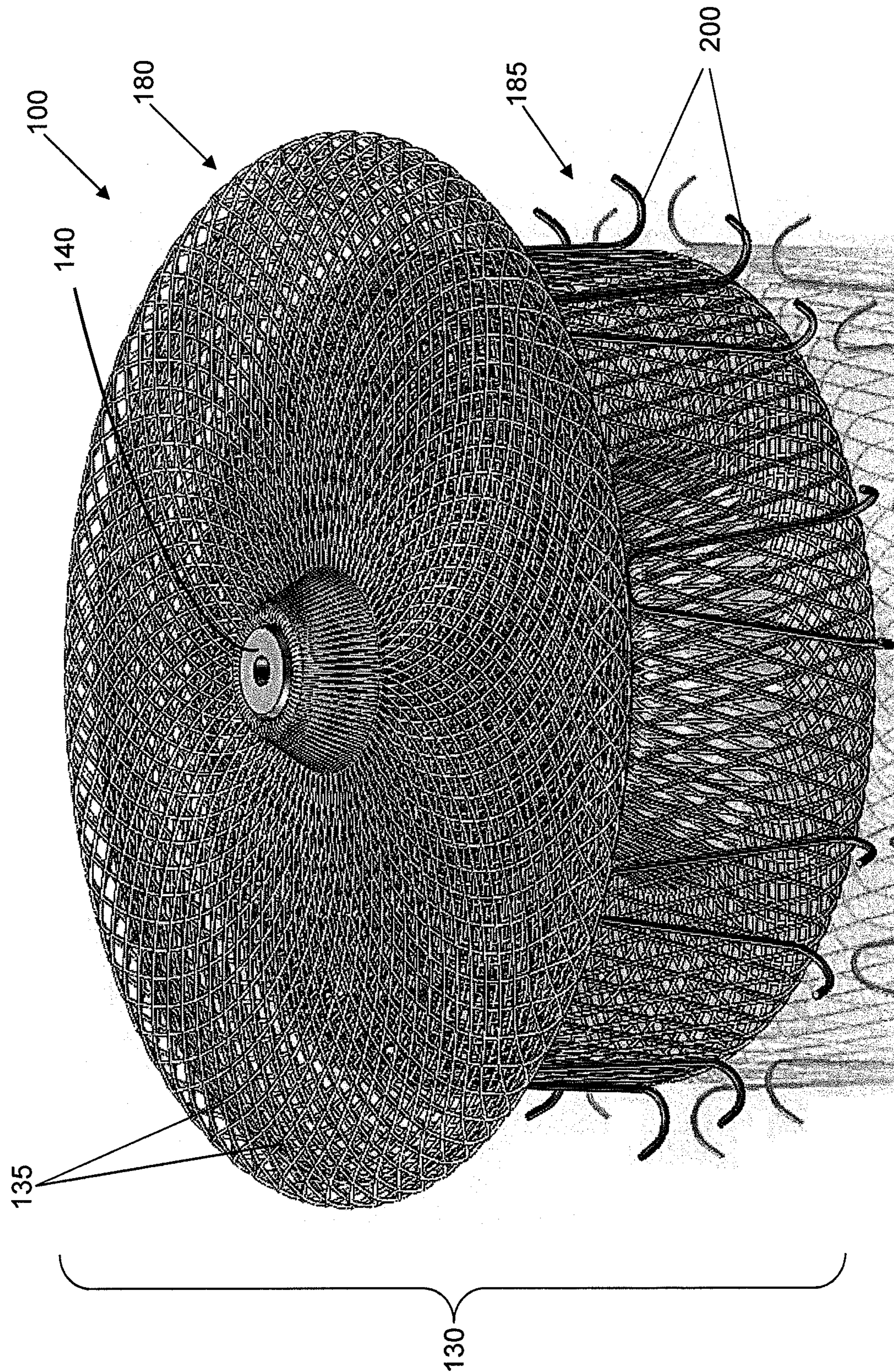


FIG. 4

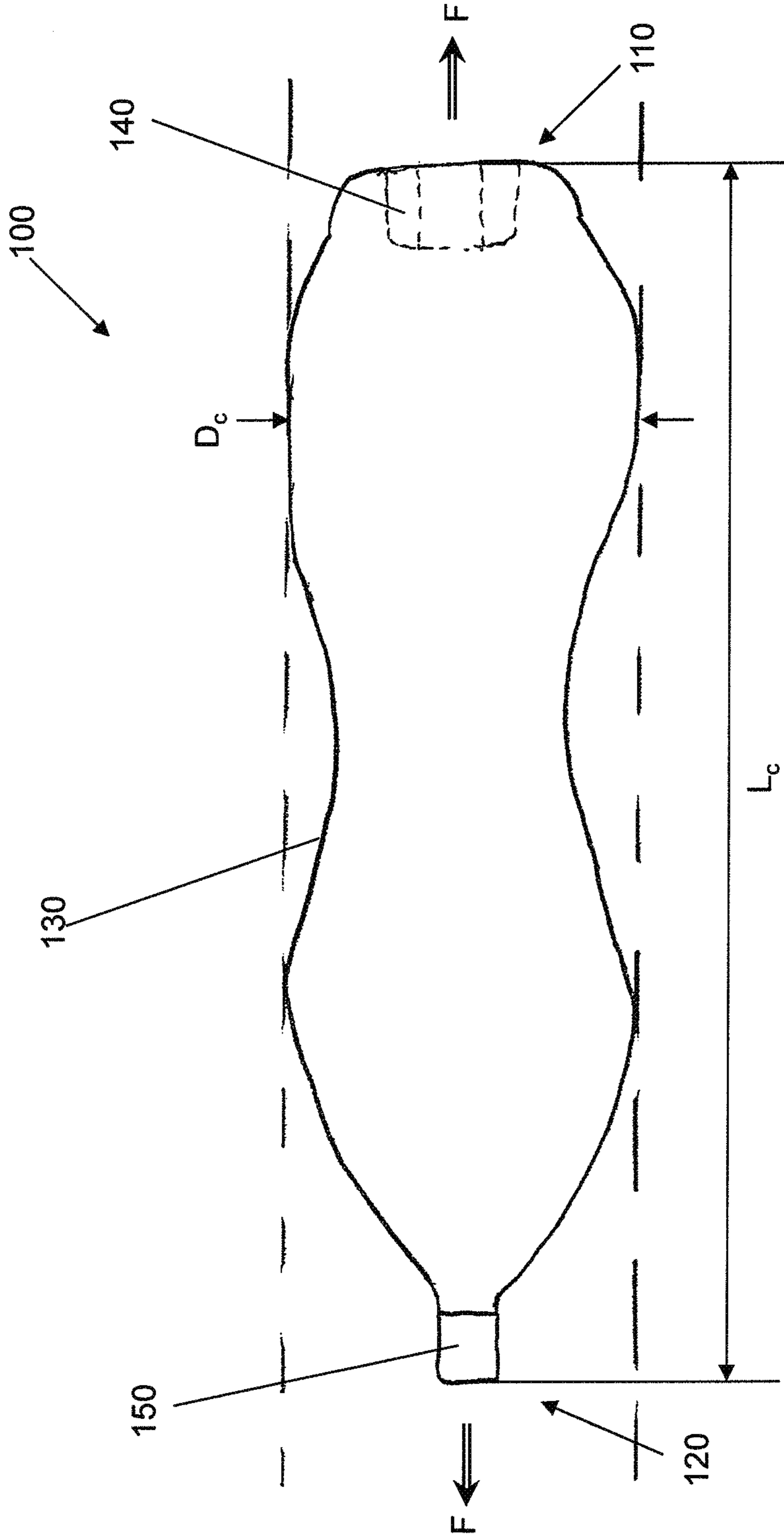


FIG. 5

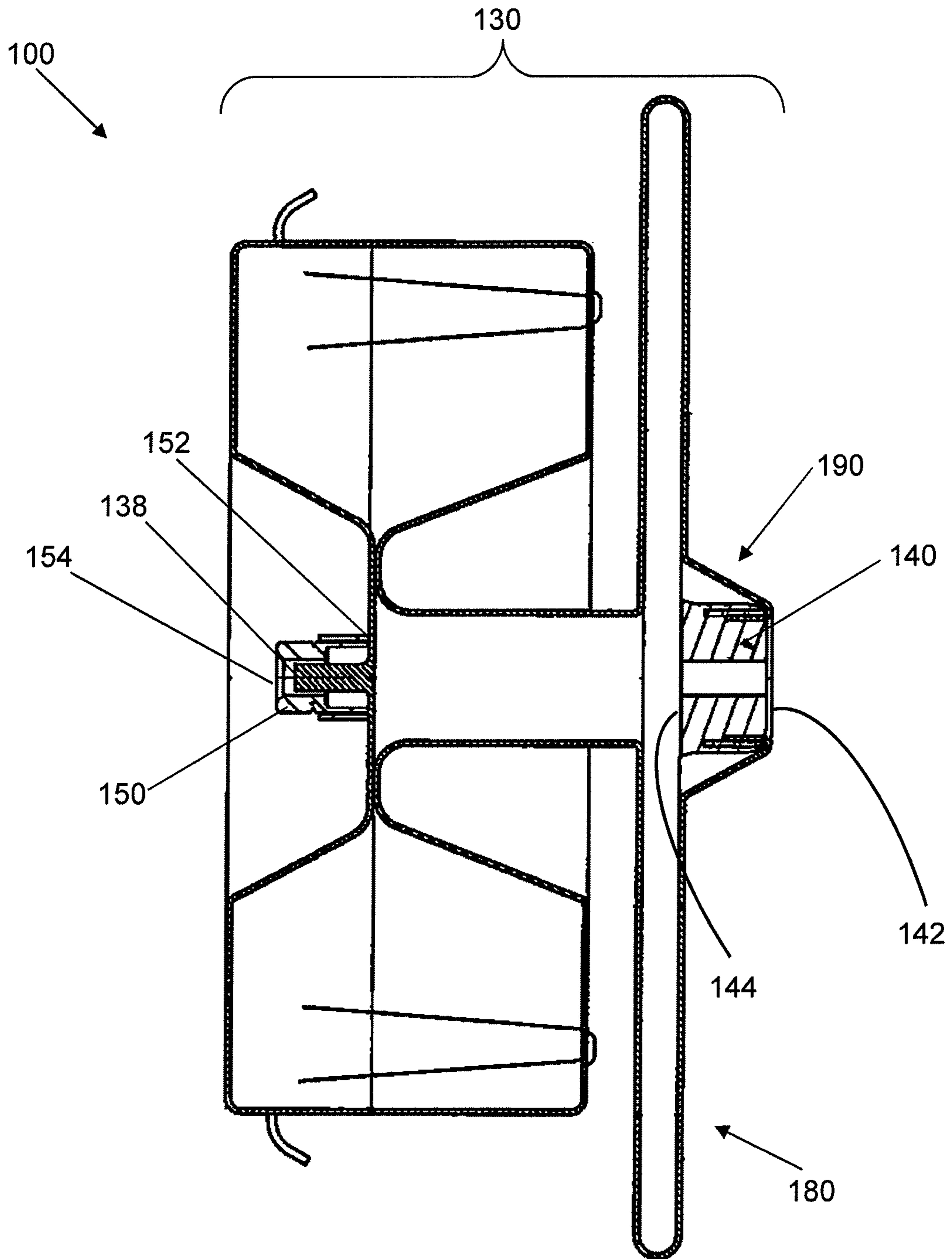


FIG. 6

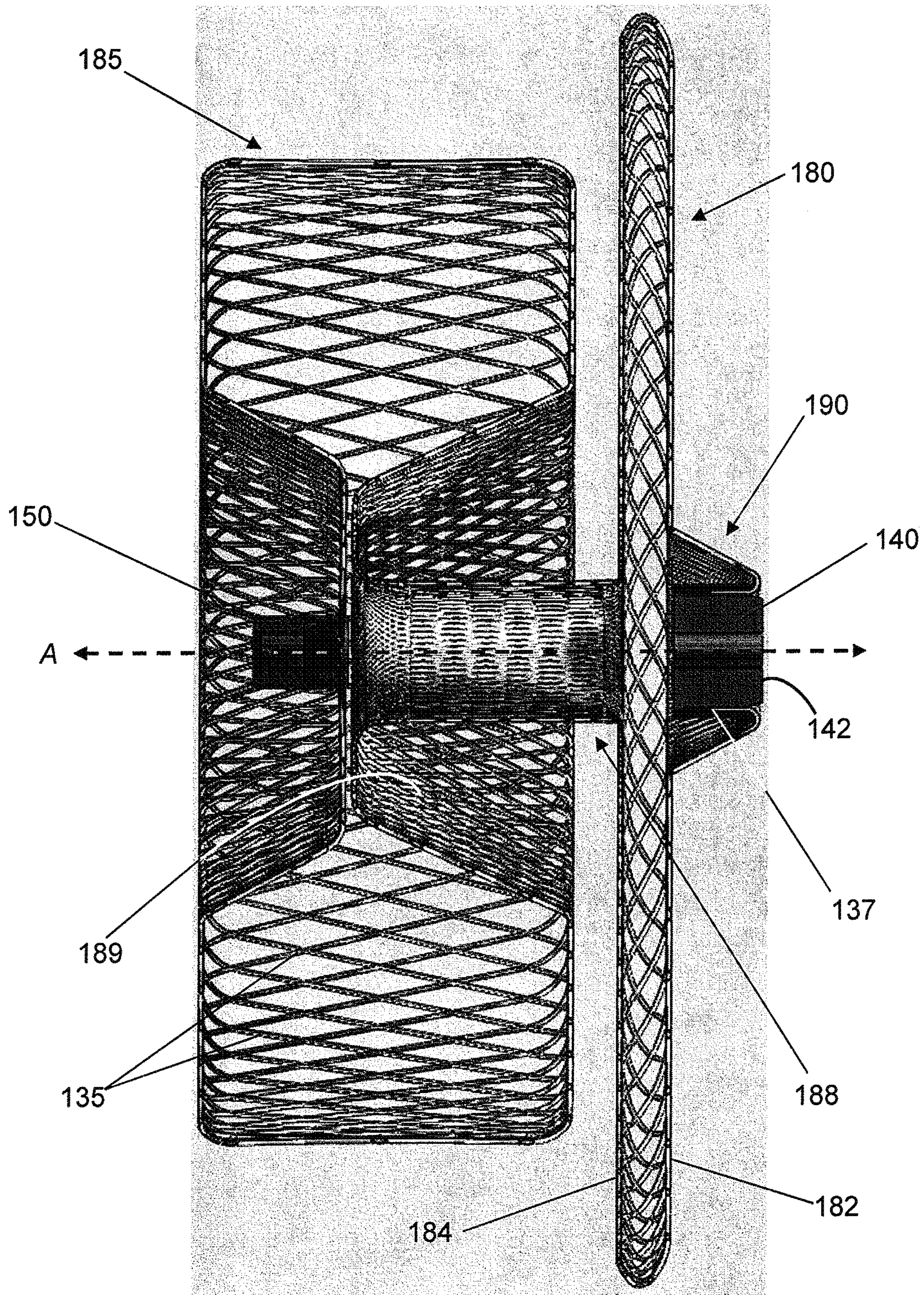


FIG. 7

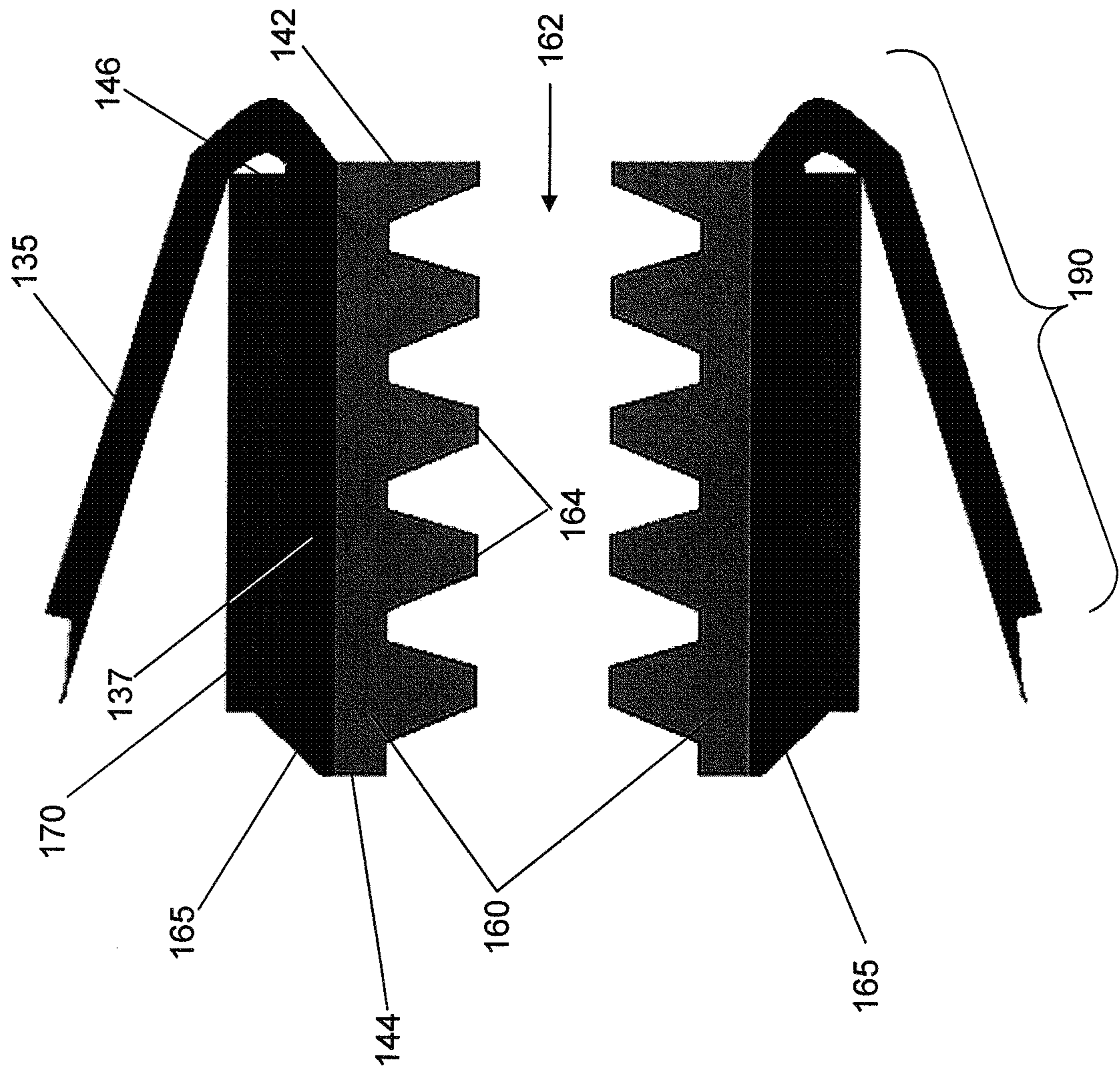


FIG. 8

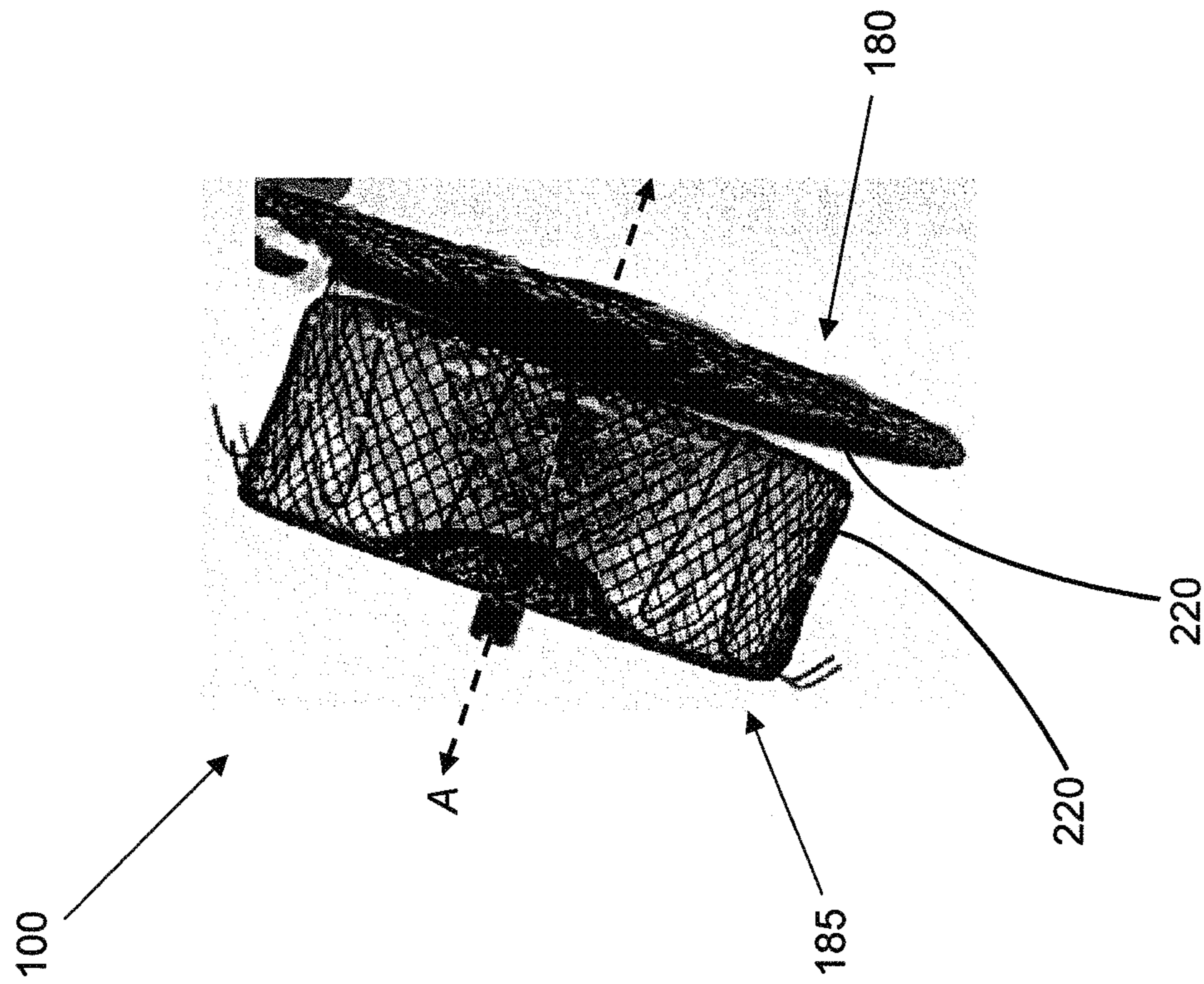


FIG. 9

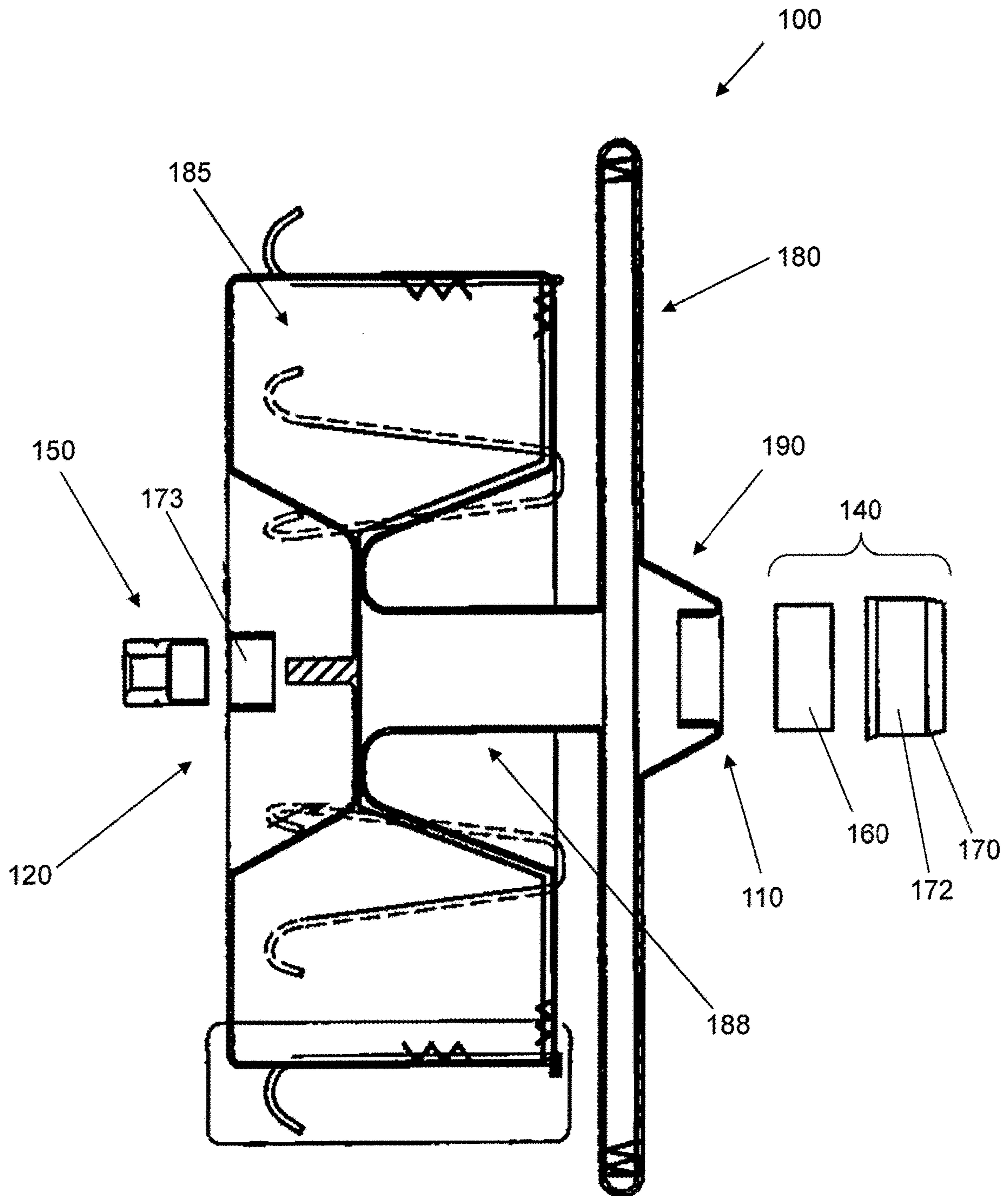


FIG. 10

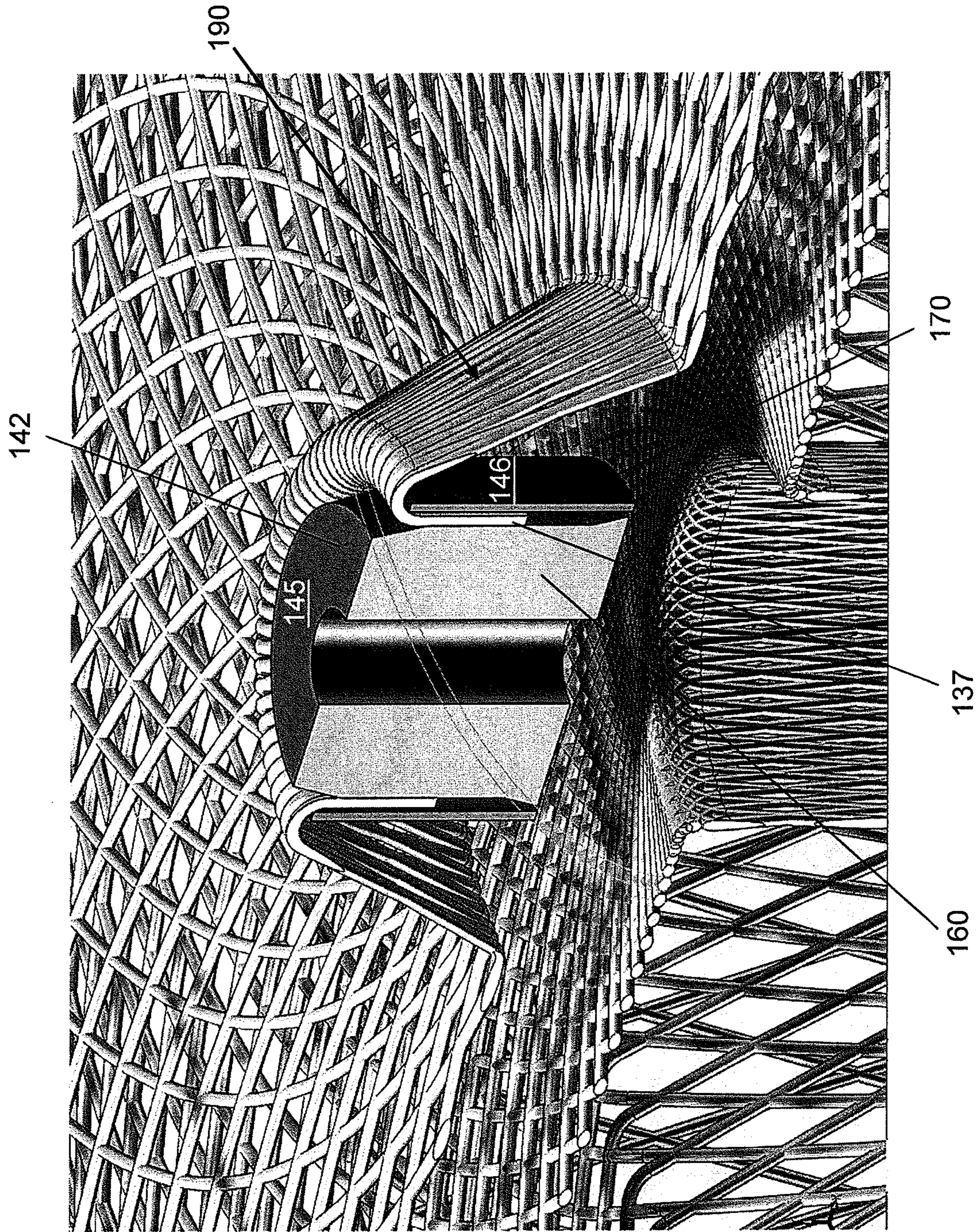


FIG. 10A

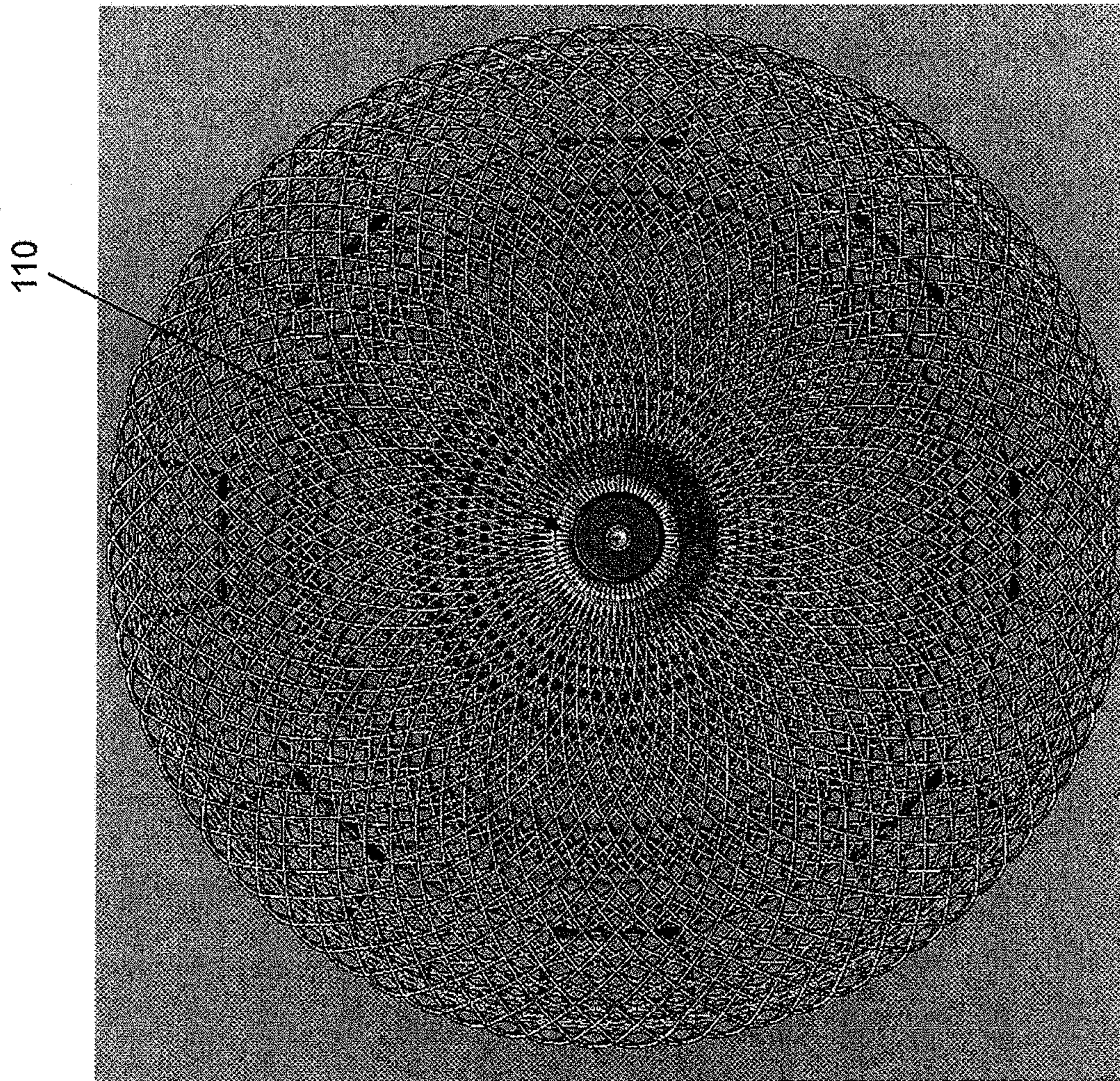


FIG. 11

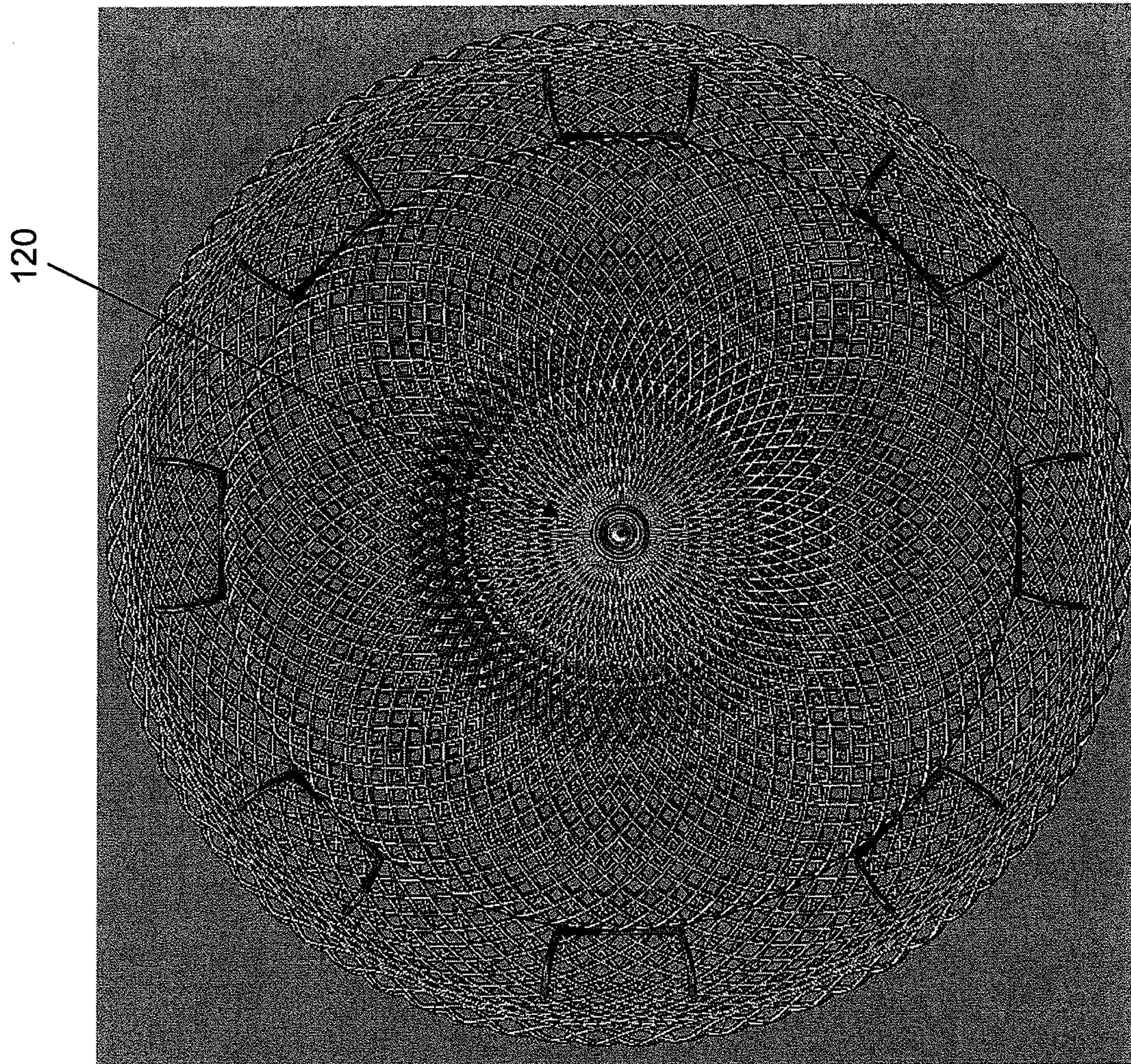


FIG. 12

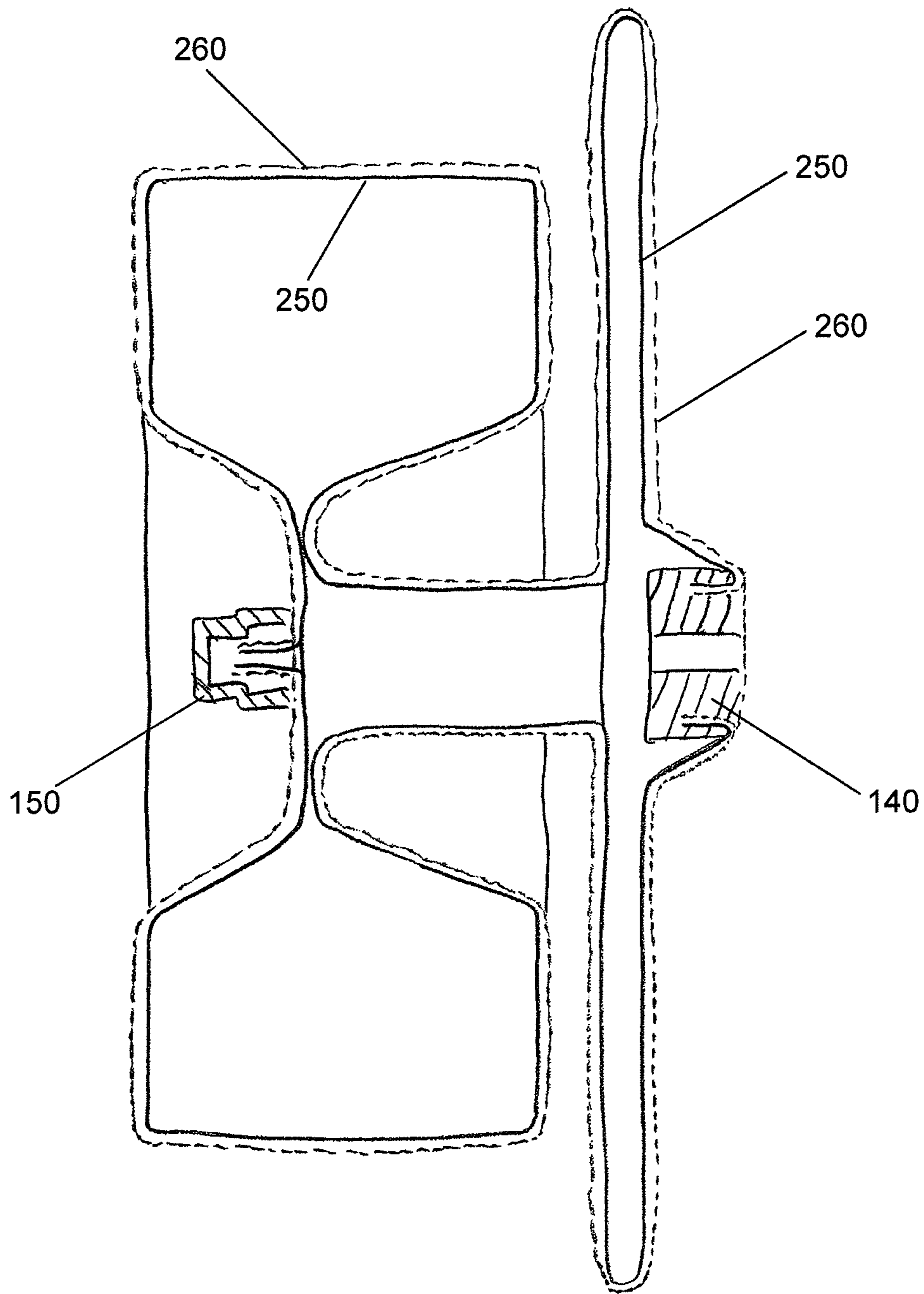
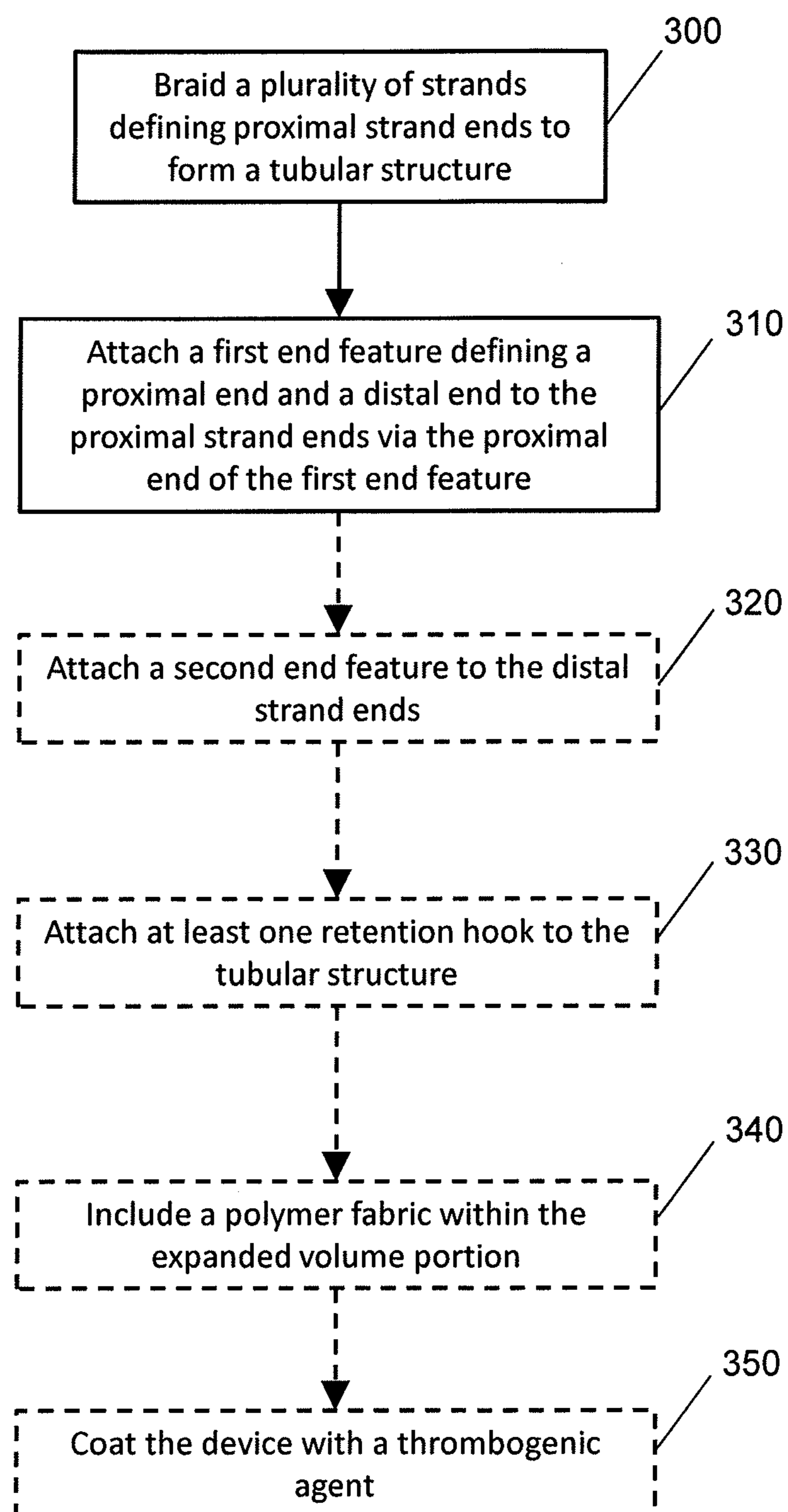


FIG. 13

FIG. 14

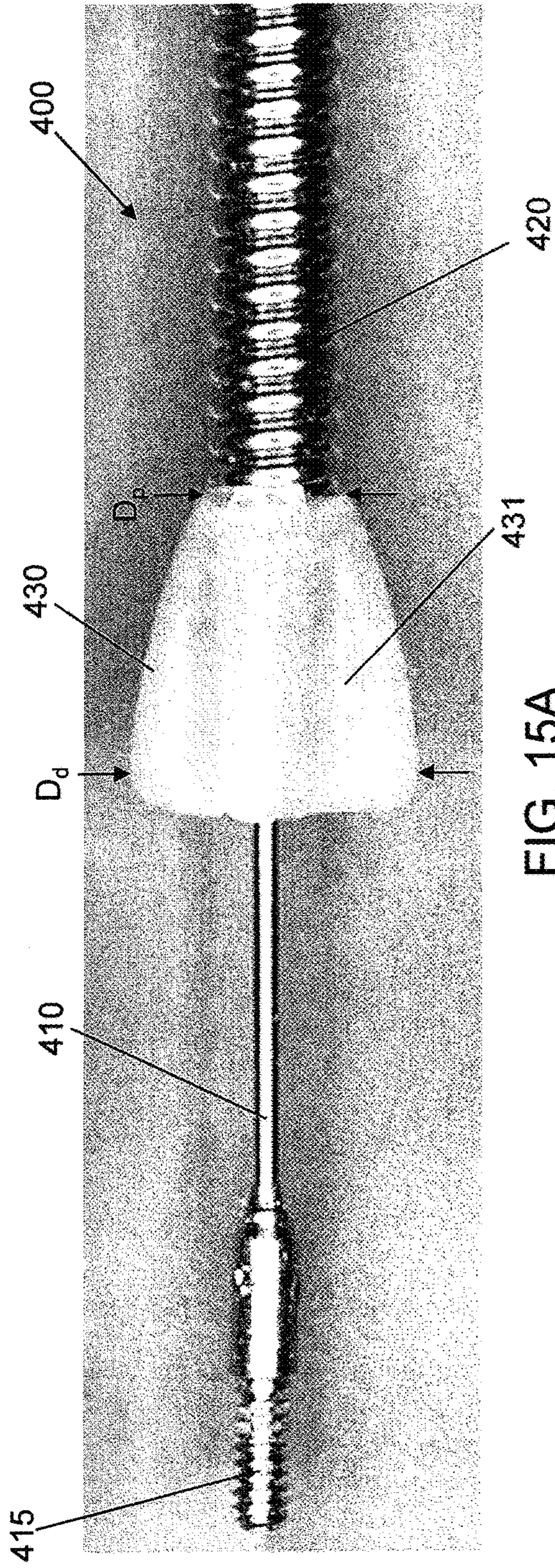


FIG. 15A

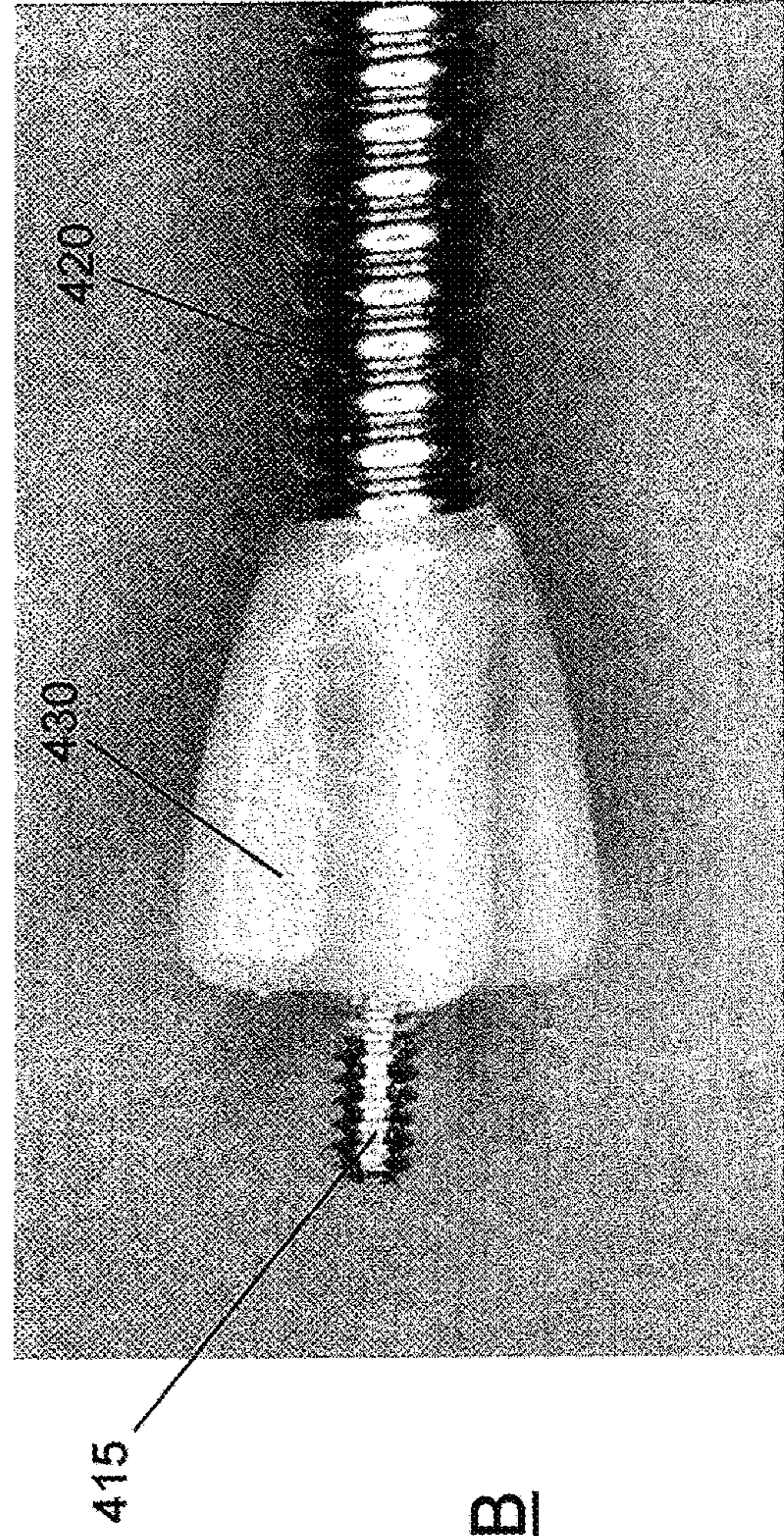


FIG. 15B

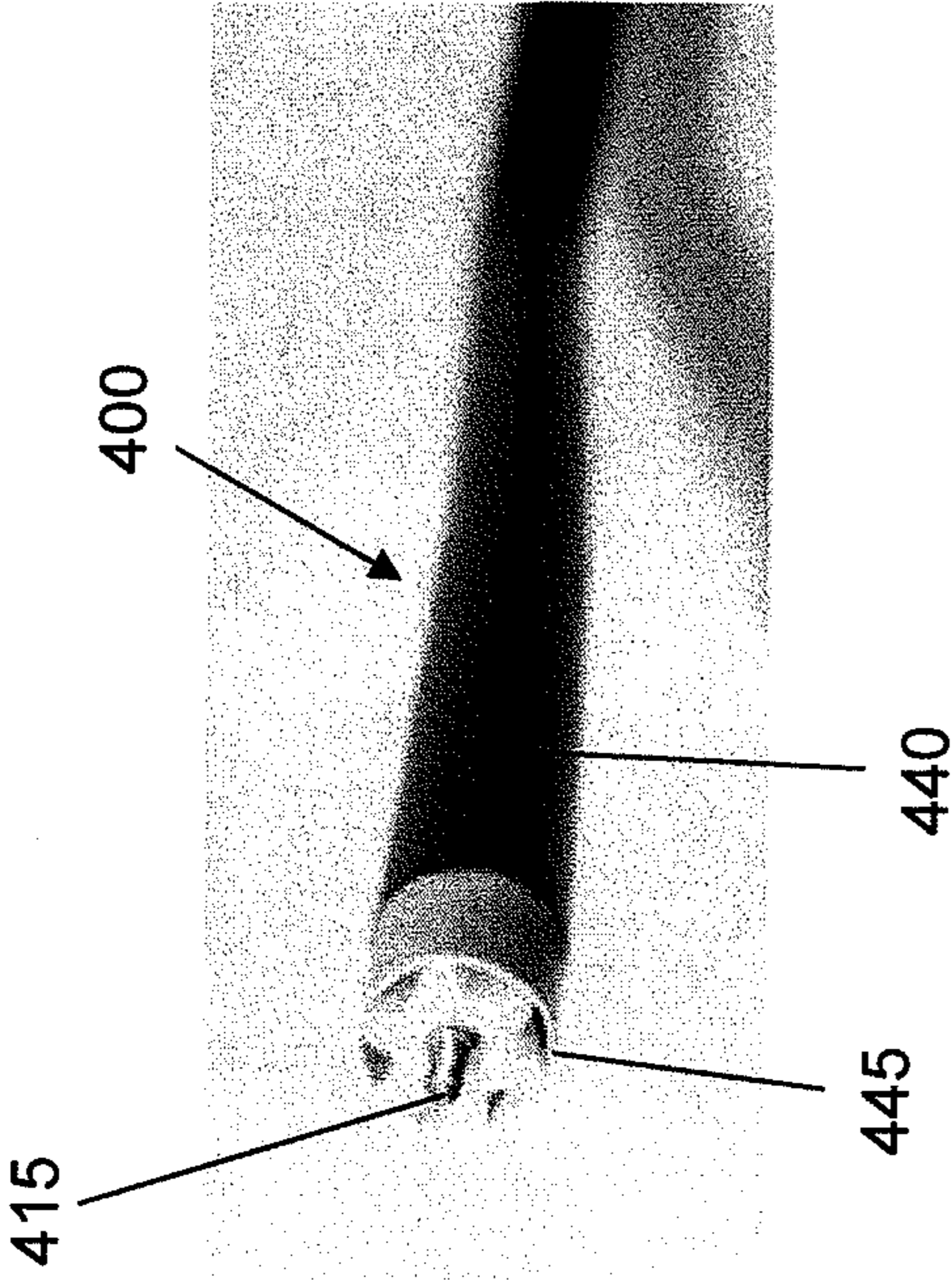


FIG. 16

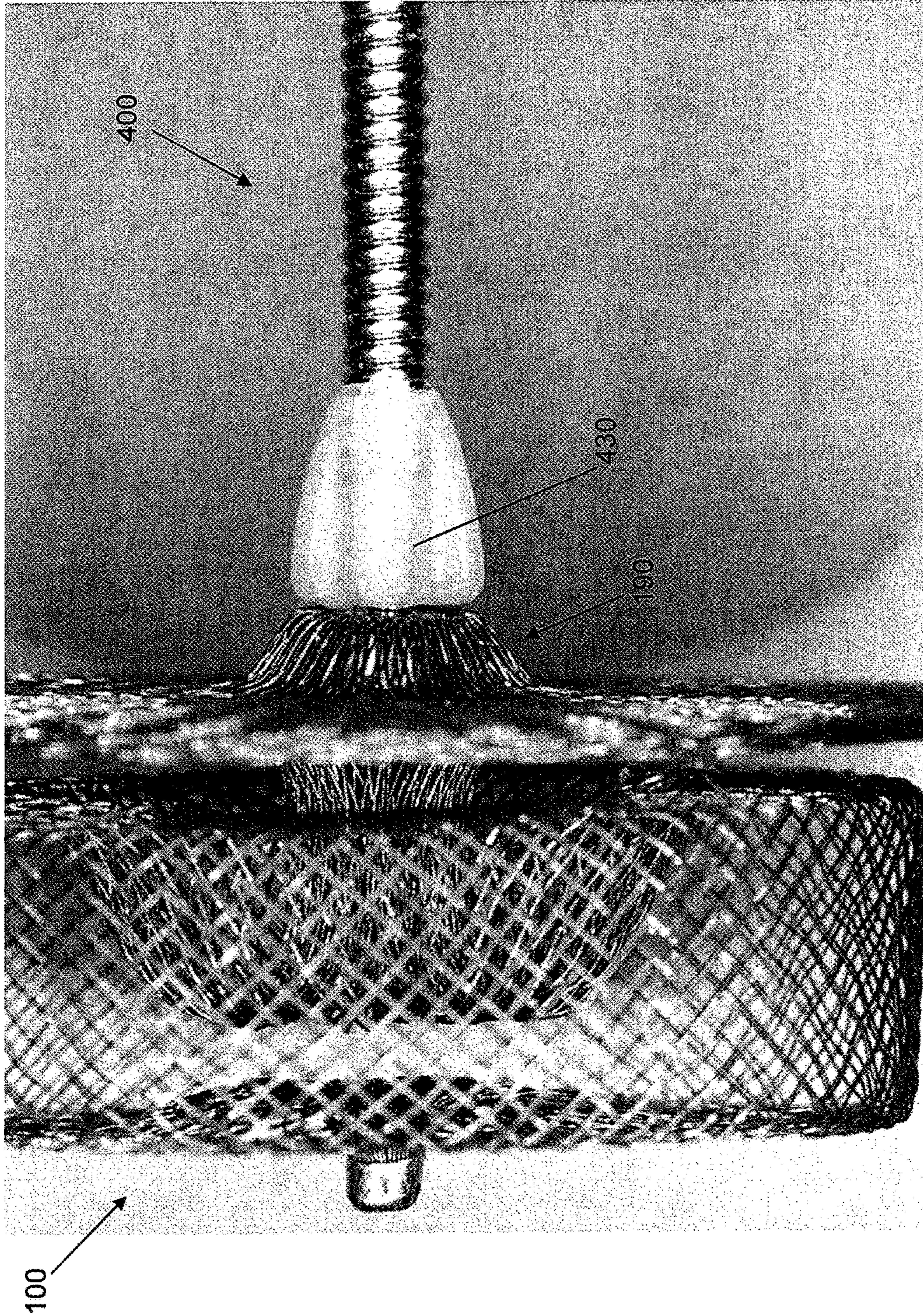


FIG. 17

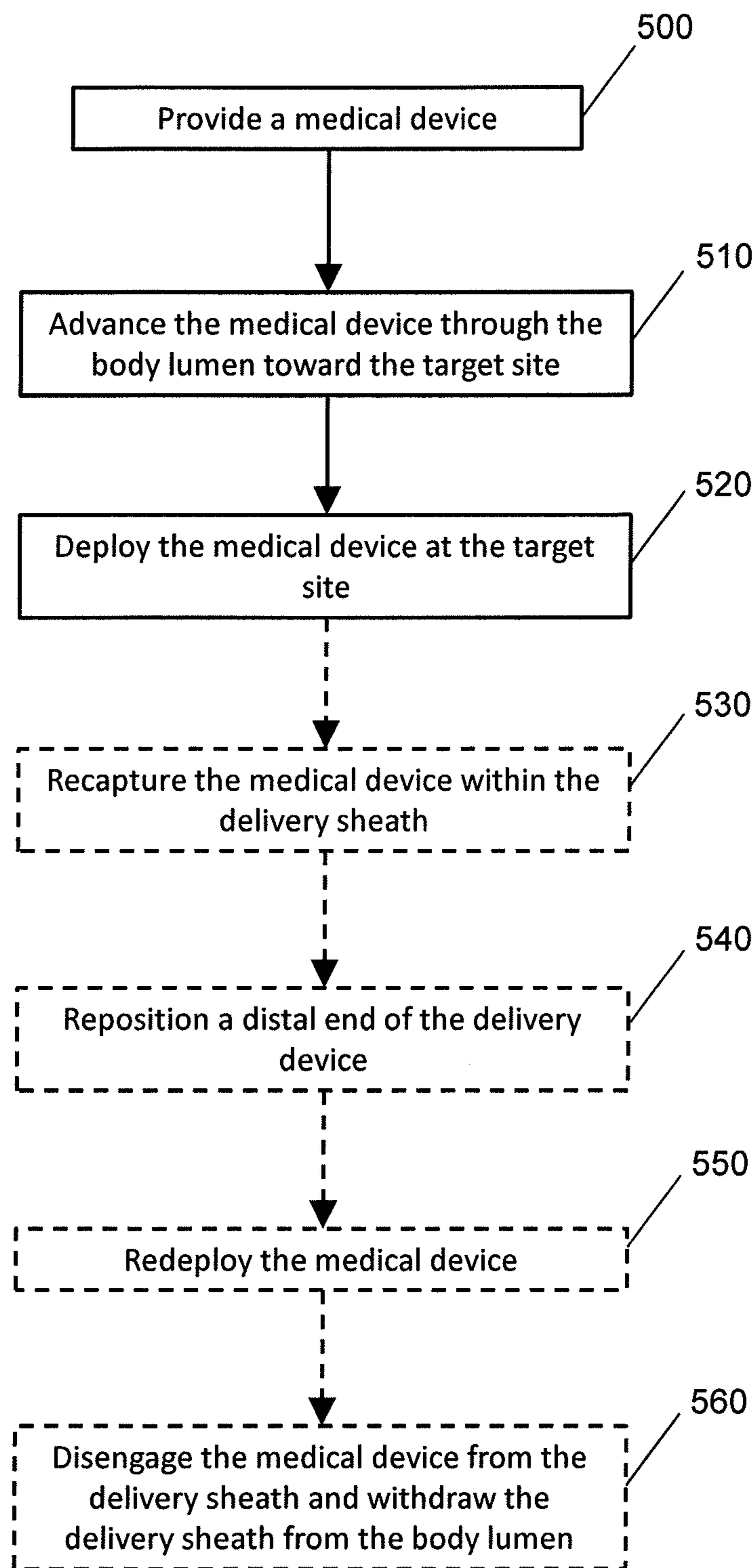


FIG. 18

**DEVICES AND METHODS FOR OCCLUDING
ABNORMAL OPENINGS IN A PATIENT'S
VASCULATURE**

CROSS-REFERENCE TO RELATED
APPLICATIONS

This application is a divisional application of U.S. patent application Ser. No. 14/243,271, published as U.S. Publication No. 2014-0214077, filed Apr. 2, 2014, which is a divisional application of U.S. patent application Ser. No. 13/300,322, now U.S. Pat. No. 8,758,389, filed on Nov. 18, 2011, which are hereby incorporated by reference in their entirety.

BACKGROUND

Field of the Invention

Embodiments of the present invention relate generally to medical devices for treating certain vascular abnormalities. In particular, embodiments are directed to medical devices and methods for occluding vascular abnormalities in which an end of the medical device is in the path of blood flow, such as closure of the Left Atrial Appendage (LAA), Atrial and Ventricular Septal Defects (ASD, VSD), and Patent Ductus Arteriosus (PDA) and the like.

Description of the Related Art

A wide variety of intravascular devices are used in various medical procedures. Certain intravascular devices, such as catheters and guidewires, are generally used simply to deliver fluids or other medical devices to specific locations within a patient's body, such as a selective site within the vascular system. Other, frequently more complex, devices are used in treating specific conditions, such as devices used in removing vascular occlusions or for treating septal defects and the like.

In certain circumstances, it may be necessary to occlude an abnormal opening in a patient's vessel, such as an abnormal opening between chambers of the heart, a channel, a hole, a cavity, or the like, so as to stop blood flow therethrough. For example, atrial fibrillation may result in the formation of a blood clot in the left atrial appendage (LAA), which may become dislodged and enter the blood stream. By occluding the LAA, the release of blood clots from the LAA may be significantly reduced, if not eliminated. Various techniques have been developed to occlude the LAA. For instance, balloon-like devices have been developed that are configured to be implanted completely within the cavity of the LAA, while surgical techniques have also been developed where the cavity of the LAA is inverted and surgically closed.

Despite these techniques, it would be advantageous to provide an improved occlusion device that offers an improved surface configuration to enhance tissue coverage or tissue in-growth, particularly on surfaces adjacent flowing blood, as well as increased flexibility, improved retention, improved thrombogenicity, and easier deployment and retrieval, thereby overcoming the shortcomings of conventional solutions for occluding abnormal openings within a patient's vasculature.

SUMMARY OF THE INVENTION

Embodiments therefore provide a medical device for occluding abnormal openings in a patient's vasculature. In

general, the medical device is configured such that an end feature of the device is recessed within a tapered transition portion formed at a respective end of the medical device. In this way, only an end surface of the end feature (e.g., a proximal end surface of the end feature at the proximal end of the medical device), or a portion of this surface, is exposed to the flow of blood through the body lumen, and tissue in-growth over the end of the device may be enhanced and facilitated.

In one embodiment, a device is provided that is configured to self-expand from a contracted state when constrained within a delivery device toward an expanded state when deployed from the delivery device for delivery to a target site within the body lumen. The medical device may include a tubular structure and a first end feature. The tubular structure may comprise a plurality of braided strands, with each braided strand comprising a proximal strand end and a distal strand end. The first end feature may define a proximal end and a distal end, and the first end feature may be configured to receive and secure the proximal strand ends via the proximal end of the first end feature. The tubular structure may comprise an expanded volume portion proximate to the first end feature and a tapered transition portion extending between the expanded volume portion and the proximal end of the first end feature. In the expanded state, the expanded volume portion of the tubular structure may define an expanded volume diameter. Moreover, in the expanded state, the tapered transition portion may define a first transition diameter proximate the expanded volume portion and a second transition diameter proximate the proximal end of the first end feature. The first transition diameter may be greater than the second transition diameter, smaller than the expanded volume diameter, and disposed between the second transition diameter and the expanded volume diameter. In addition, the second transition diameter may be substantially equal to a diameter of the first end feature. In some cases, the second transition diameter may be sized to facilitate tissue growth over a proximal end of the medical device.

Embodiments of the medical device may also include a second end feature configured to receive and secure the distal strand ends of the plurality of braided strands. The medical device may define a central axis extending between the first end feature and the second end feature, and the expanded volume portion may define at least one surface that is substantially perpendicular to the central axis. In some cases, the expanded volume portion may define two surfaces that are substantially perpendicular to the central axis. The second end feature may define a proximal end and a distal end, and the second end feature may be configured to receive and secure the distal strand ends via the distal end of the second end feature.

In some cases, the expanded volume portion may be a first expanded volume portion and the tapered transition portion may be a first tapered transition portion. The tubular structure may further include a second expanded volume portion displaced from the first expanded volume portion and proximate the second end feature and a second tapered transition portion extending between the second expanded volume portion and the distal end of the second end feature. The expanded volume portion may be disk shaped.

The expanded volume portion may be a first expanded volume portion, and the tubular structure may further comprise a second expanded volume portion proximate the second end feature. The first expanded volume portion may be disk shaped, and the second expanded volume portion may be cylindrically shaped. The first expanded volume

portion and the second expanded volume portion may be connected by a flexible connector such that the first and second expanded volume portions can articulate with respect to each other.

The second expanded volume portion may, in some cases, comprise a cone shaped end surface affixed to the connector. In addition, a plurality of hooks may be disposed on and may extend radially and axially outward from the second expansion volume portion. The hooks may be configured to engage body tissue when the device is moved along a central axis of the medical device in a proximal direction.

At least one of the first and second expanded volume portions may comprise a polymer fabric disposed therein, and at least a portion of the polymer fabric may extend substantially perpendicularly to the axis. The polymer fabric may be secured to a respective one of the first and second expanded volume portions.

In some embodiments, the medical device may define a proximal end and a distal end, and the proximal end of the first end feature may substantially coincide with the proximal end of the medical device. The medical device may be configured to occlude a vessel, cavity, hole, septal defect, or lumen in a body. For example, the medical device may be configured to occlude the left atrial appendage of the heart and to prevent thrombus from escaping therefrom.

In some cases, the tubular structure may be a first tubular structure, and the medical device may further comprise a second tubular structure comprising a second plurality of braided strands. The second plurality of braided strands may be comprised of a metal or polymer. The braided strands may comprise a metal having elastic properties, and/or the braided strands may comprise a shape memory alloy. The expanded volume portion may be heatset in a mold to memorize its expanded state.

The medical device may further comprise a polymer fabric disposed within the expanded volume portion, and the polymer fabric may be polyester.

In other embodiments, a medical device may be provided that is configured to self-expand from a contracted state when constrained within a delivery device toward an expanded state when deployed from the delivery device for delivery to a target site within the body lumen. The medical device may comprise a tubular structure and a first end feature. The tubular structure may comprise a plurality of braided strands, and each braided strand may comprise a proximal strand end and a distal strand end. The first end feature may have a proximal end and a distal end, and the first end feature may be configured to receive and secure the proximal strand ends via the proximal end of the first end feature. Moreover, the proximal end of the first end feature may comprise a proximal end surface, a distal end surface, and a circumferential surface extending between the proximal and distal end surfaces. The tubular structure may comprise an expanded volume portion proximate to the first end feature and a tapered transition portion extending between the expanded volume portion and the proximal end of the first end feature. In the expanded state, the proximal strand ends may be secured to the first end feature such that the transition portion substantially surrounds the circumferential surface of the first end feature and only the proximal end surface of the first end feature or a portion of the proximal end surface is exposed to fluid flow through the body lumen.

In still other embodiments, a medical device may be provided that is configured to self-expand from a contracted state when constrained within a delivery device toward an expanded state when deployed from the delivery device for

delivery to a target site within the body lumen. The medical device may include a tubular structure comprising a plurality of braided strands, and each braided strand may comprise a proximal strand end and a distal strand end. The medical device may further include a first end feature having a proximal end and a distal end, where the first end feature is configured to receive and secure the proximal strand ends via the proximal end of the first end feature. The tubular structure may comprise an expanded volume portion proximate to the first end feature and a tapered transition portion extending between the expanded volume portion and the proximal end of the first end feature. In the expanded state, the proximal strand ends may be secured to the first end feature such that the proximal strand ends are at least partially inverted at the proximal end of the first end feature.

In still other embodiments, a method of making a medical device for placement in a body lumen is provided. The method includes braiding a plurality of strands defining proximal strand ends to form a tubular structure and attaching a first end feature defining a proximal end and a distal end to the proximal strand ends via the proximal end of the first end feature. The medical device may be configured to self-expand from a contracted state when constrained within a delivery device toward an expanded state when deployed from the delivery device for delivery to a target site within the body lumen. The tubular structure may comprise an expanded volume portion proximate to the first end feature and a tapered transition portion extending between the expanded volume portion and the proximal end of the first end feature. In the expanded state, the expanded volume portion of the tubular structure may define an expanded volume diameter. Furthermore, in the expanded state, the tapered transition portion may define a first transition diameter proximate the expanded volume portion and a second transition diameter proximate the proximal end of the first end feature. The first transition diameter may be greater than the second transition diameter, smaller than the expanded volume diameter, and disposed between the second transition diameter and the expanded volume diameter. The second transition diameter may be substantially equal to a diameter of the first end feature.

In still other embodiments, a method of delivering a medical device is provided. The method includes providing a medical device configured to self-expand from a contracted state when constrained within a delivery device toward an expanded state when deployed from the delivery device for delivery to a target site within the body lumen, where the medical device is configured as described above. The medical device may be advanced through a body lumen toward the target site and deployed at the target site.

BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing features and advantages of embodiments of the invention will become apparent to those skilled in the art from the following detailed description of a preferred embodiment, especially when considered in conjunction with the accompanying drawings in which like numerals in the several views refer to corresponding parts.

FIG. 1 illustrates a conventional medical device that includes protruding end clamps;

FIG. 2 is a schematic side view of a medical device in an expanded state according to an exemplary embodiment;

FIG. 3 illustrates tissue growth over the proximal end of an implanted medical device according to an exemplary embodiment;

5

FIG. 4 is a schematic perspective view of the medical device of FIG. 2 in an expanded state from the proximal end according to an exemplary embodiment;

FIG. 5 is a schematic side view of the medical device of FIG. 2 in a contracted state according to an exemplary embodiment;

FIG. 6 is a simplified cross-sectional view of the medical device of FIG. 2 according to an exemplary embodiment;

FIG. 7 is a cross-sectional view of the medical device of FIG. 2 according to an exemplary embodiment;

FIG. 8 is a close-up cross-sectional view of a first end feature of the medical device according to an exemplary embodiment;

FIG. 9 illustrates a medical device that includes a polymer fabric in each of the first and second expanded volume portions according to an exemplary embodiment;

FIG. 10 is a simplified cross-sectional view of the medical device of FIG. 6 in exploded form according to an exemplary embodiment;

FIG. 10A is a perspective cross-sectional view of the first end feature of the medical device of FIG. 10 according to an exemplary embodiment;

FIG. 11 illustrates the proximal end of a medical device according to an exemplary embodiment;

FIG. 12 illustrates the distal end of a medical device according to an exemplary embodiment;

FIG. 13 is a schematic illustration of a medical device including first and second tubular structures (an inner and an outer layer) according to an exemplary embodiment;

FIG. 14 illustrates a flowchart for a method for making a medical device for occluding an abnormal opening in the body lumen;

FIG. 15A is a schematic illustration of a delivery device in a first position according to an exemplary embodiment;

FIG. 15B is a schematic illustration of a delivery device in a second position according to an exemplary embodiment;

FIG. 16 is a schematic illustration of the delivery device of FIGS. 15A and 15B showing the guide member disposed within the lumen of a delivery catheter;

FIG. 17 is a schematic illustration of the delivery device of FIG. 15A engaged to the proximal end of the medical device according to an exemplary embodiment; and

FIG. 18 illustrates a flowchart for a method for delivering a medical device.

DETAILED DESCRIPTION

Embodiments of the present invention now will be described more fully hereinafter with reference to the accompanying drawings, in which some, but not all embodiments of the invention are shown. Indeed, the invention may be embodied in many different forms and should not be construed as limited to the embodiments set forth herein; rather, these embodiments are provided so that this disclosure will satisfy applicable legal requirements. Like numbers refer to like elements throughout.

In general, embodiments of a medical device are described that provide an end feature that is recessed within a tapered transition portion formed at a respective end of the medical device, such that the end feature does not protrude from the respective end of the device. In this way, the medical device may be safely and easily deployed at target sites in certain locations of the patient's vasculature where blood flow may occur across one or both ends by providing a surface configuration that facilitates tissue coverage while reducing the risk of a thrombotic embolism. For example, in conventional devices, such as the device 10 shown in FIG.

6

1, an end clamp 20 may be provided at a proximal end of the medical device that protrudes outwardly from the braided structure 30. As a result, blood flow in the direction of the arrow 40 may be disrupted in the area of the end clamp 20.

Because of the smooth surface of the clamp and its location in the stream of blood flow, tissue growth on the clamp may not occur as quickly as it occurs over other surfaces of the device. There is always a risk of clot formation over device surfaces prior to tissue incorporation, so anti-clotting medications may be prescribed to protect the patient during a period of time until tissue coverage is complete. Embolisms may form and dislodge from uncovered surfaces and may travel through the patient's vasculature, putting the patient at risk, so it is preferable to have device surfaces where tissue coverage is facilitated. Further examples of medical devices are provided in U.S. Publication No. US 2009/0171386 titled "Percutaneous Catheter Directed Intravascular Occlusion Devices" and filed on Dec. 28, 2007, which is incorporated by reference herein in its entirety.

Accordingly, embodiments of the medical device 100, such as shown in FIG. 2, are configured such that one or both ends 110, 120 of the device encourage formation of tissue across substantially the entire area of the respective end that is exposed to the blood flow, such that the risk of a thrombotic embolism may be minimized. An illustration of a device that has been placed in the body lumen at a target site for a period of time, showing the growth of tissue 50 over at least the proximal end 110 of the device, is provided in FIG. 3. Moreover, embodiments of the present invention provide for attachment of the end feature(s) in such a way that radial expansion and contraction of the medical device as the medical device is moved between contracted and expanded states is facilitated as compared to conventional devices, as described in greater detail below.

It is understood that the use of the term "target site" is not meant to be limiting, as the medical device may be configured to treat any target site, such as an abnormality, a vessel, an organ, an opening, a chamber, a channel, a hole, a cavity, or the like, located anywhere in the body. The term "vascular abnormality," as used herein is not meant to be limiting, as the medical device may be configured to bridge or otherwise support a variety of vascular abnormalities. For example, the vascular abnormality could be any abnormality that affects the shape of the native lumen, such as an LAA, an atrial septal defect, a lesion, a vessel dissection, or a tumor. Embodiments of the medical device may be useful, for example, for occluding an LAA, ASD, VSD, or PDA, as noted above. Furthermore, the term "lumen" is also not meant to be limiting, as the vascular abnormality may reside in a variety of locations within the vasculature, such as a vessel, an artery, a vein, a passageway, an organ, a cavity, or the like. For ease of explanation, the examples used herein refer to the occlusion of an LAA. As used herein, the term "proximal" refers to a part of the medical device or the delivery device that is closest to the operator, and the term "distal" refers to a part of the medical device or the delivery device that is farther from the operator at any given time as the medical device is being delivered through the delivery device.

According to one embodiment of the present invention for forming the medical device 100, a plurality of strands may be braided together to form a tubular structure. Although the strands are described as being braided, it is understood that according to additional embodiments of the present invention, the medical device 100 may be formed by braiding, interweaving, knitting, or otherwise combining filamentary materials together, such as by using a conventional braiding

machine. These filamentary materials may include, for example, fibers, thread, yarn, cable, metallic wires, polymer monofilament or multifilament strands, and combinations of these materials, any of which are referenced herein as “strands,” and such terms may be used interchangeably. The strands may be comprised of any material, such as natural materials, polymers, metals, metallic alloys, or combinations of the same. The strands may be braided to have a predetermined pick and pitch to define openings or fenestrations so as to vary the impedance of blood flow there-through.

In some cases, other techniques may be used to form the tubular structure. For example, the tubular structure could be etched or laser cut from a tube such as to form an interstice geometry, or the tubular structure could comprise an occlusion material coupled to a scaffolding structure or a plurality of slices of a tubular member coupled together, such as via gluing. Moreover, it is understood that the medical device **100** may comprise one or more layers of occluding material such that the medical device may include a variety of occluding materials capable of at least partially inhibiting blood flow therethrough in order to facilitate the formation of thrombus.

According to one embodiment, the occluding material of the tubular structure **130**, shown in FIG. 4, is a metal fabric including a plurality of strands **135**, such as two sets of essentially parallel generally helical strands, with the strands of one set having a “hand,” or a direction of rotation, opposite that of the other set.

The pitch of the strands **135** (the angle defined between the turns of the strands and the axis of the braid) and the pick of the fabric (the number of wire strand crossovers per unit length) may be adjusted as desired for a particular application. The wire strands of the metal fabric used in one embodiment of the present method may be formed of a material that is both resilient and can be heat treated to substantially set a desired shape. Materials which may be suitable for this purpose include a cobalt-based low thermal expansion alloy referred to in the field as Elgiloy, nickel-based high temperature high-strength “superalloys” commercially available from Haynes International under the trade name Hastelloy, nickel-based heat treatable alloys sold under the name Incoloy by International Nickel, and a number of different grades of stainless steel. An important consideration in choosing a suitable material for the wires strands is that the wires retain a suitable amount of the deformation induced by the molding surface (as described below) when subjected to a predetermined heat treatment and elastically return to said molded shape after substantial deformation.

One class of materials which meets these qualifications is so-called shape memory alloys. One particular shape memory alloy that may be used is Nitinol. Nitinol alloys are also highly elastic and are said to be “superelastic,” or “pseudoelastic.” This elasticity may allow the device to return to a preset expanded configuration for deployment following passage in a distorted form through a delivery catheter. Moreover, other suitable materials include those that are compatible with magnetic resonance imaging (MRI), as some materials may cause heat or torque resulting from performing MRI, and some materials may distort the MRI image. Thus, metallic and/or non-metallic materials that reduce or eliminate these potential problems resulting from using MRI may be employed. Further examples of materials and manufacturing methods for medical devices with shape memory properties are provided in U.S. Publication No. 2007/0265656 titled “Multi-layer Braided Struc-

tures for Occluding Vascular Defects” and filed on Jun. 21, 2007, which is incorporated by reference herein in its entirety.

In some embodiments, one or more layers of fabric may be employed to form a medical device, as described in greater detail below. For example, two layers of metal fabric could be separately woven into tubular structures, with one tubular structure coaxially disposed within the second tubular structure. For further discussion regarding a multi-layer braided device and techniques for fabricating such a device, see U.S. Patent Appl. Publ. No. 2007/0168019 to Amplatz et al., which is hereby incorporated in its entirety by reference.

The tubular structure **130** used to fabricate medical devices **100** according to one embodiment of the present invention may use wire strands ranging in diameter from 0.0015 in. to 0.005 in., preferably in the range of 0.003 to 0.0045 in. The number of wires in the tubular braid may vary from 36 to 144 but preferably is in the range of 72 to 144. The pick count of the braid may vary from 30 to 100. The fabric may thus have an average area between supporting fibers of between approximately 0.0016 sq. cm. and 0.25 sq. cm.

Once an appropriately sized tubular structure is obtained, the fabric may be deformed to generally conform to a surface of a molding element. For example, the tubular structure **130** may be deformed to define one or more expanded volume portions **180**, **185**, as shown in FIG. 4. Deforming the fabric will reorient the relative positions of the wire strands of the metal fabric from their initial order to a second, reoriented configuration. The shape of the molding element should be selected to deform the fabric into substantially the shape of the desired medical device when unconstrained. Once the molding element is assembled with the metal fabric generally conforming to a molding surface of that element, the fabric can be subjected to a heat treatment while it remains in contact with that molding surface. After the heat treatment, the fabric may be removed from contact with the molding element and should substantially retain its shape in a deformed state.

In this way, a medical device **100** may be formed that is configured to self-expand from a contracted state when constrained within a delivery device (such as a catheter, represented by dashed lines in FIG. 5) toward an expanded state when deployed from the delivery device for delivery to a target site within the body lumen (shown in FIG. 2). In the contracted state, the medical device **100** may define a length L_c , and in the expanded state the medical device may define a length L_e . The medical device **100** may be moved to the contracted state, for example, when the ends **110**, **120** of the device are pulled away from each other and/or a radial constraint is applied to the device. In other words, as shown in FIG. 5, the application of a tensile force F on the ends of the device **100** may serve to collapse the overall outer diameter D_e of the device such that it may achieve a reduced diameter D_c , allowing the device to be received within a lumen of a delivery device in the contracted state (FIG. 5) for delivery to the target site. Thus, in this example, the delivery device (e.g., a catheter) applies the radial constraint to maintain the medical device **100** in the contracted state.

The medical device **100** may be configured, however, such that, when the radial constraint is removed, the device can self-expand to the expanded state shown in FIG. 2. For example, as the medical device **100** is unsheathed from the delivery device, portions of the medical device that are no longer constrained by the delivery device may self-expand and freely return to the expanded state, and once the medical device has been fully deployed from the delivery device

proximate the target site, the medical device will at least partially assume the expanded state. For example, the vessel diameter or the diameter of the opening in which the medical device **100** is inserted may limit complete return to the expanded state.

Thus, a medical device having a predetermined shape may be collapsed by longitudinally stretching the medical device (as illustrated in FIG. 5) for inserting the device into the lumen of a delivery device (e.g., a guide catheter or delivery sheath). The delivery device may then be positioned and advanced in a patient's body such that the distal end of the delivery device is adjacent to the target site (e.g., straddling the abnormal opening). The medical device **100** may be advanced through the delivery device such that the distal end of the medical device is near the distal end of the delivery device. Thus, as the medical device is deployed from the distal end of the delivery device, the diameter of the medical device is allowed to self-expand at the target site, e.g., to occlude the abnormal opening in the patient's vasculature.

A simplified cross-section of one embodiment of the medical device is shown in FIG. 6, with a more detailed cross-section depicting the braided strands from which the tubular structure is formed shown in FIG. 7. A simplified exploded view of the medical device **100** is shown in FIG. 10. With reference to FIGS. 4, 6, 7, and 10, embodiments of the medical device **100** comprise a tubular structure **130** comprising a plurality of braided strands **135** including proximal strand ends **137**. A first end feature **140** is provided that includes a proximal end **142** and a distal end **144**. The first end feature **140** may be configured to receive and secure the proximal strand ends **137** via the proximal end of the first end feature. In some cases, as shown in FIGS. 8 and 10, the first end feature **140** may include an inner bushing **160** (e.g., a stainless steel bushing) in which an inner lumen **162** is formed, and internal threads **164** may be defined on an inner surface of the threaded inner bushing **160** for receiving corresponding threads of a pusher wire of a delivery system, for example. The plurality of strands **135** may be placed around the threaded inner bushing **160**, as shown, and another, larger diameter outer bushing **170** (e.g., a platinum/iridium alloy bushing) may be disposed around the inner bushing **160**, such that the proximal ends **137** of the braided strands **135** are secured (e.g., tightly wedged) between the inner and outer bushings **160**, **170**. The proximal ends **137** of the braided strands **135** may then be secured, e.g., by laser welding such that a weld **165** is created to fuse both the inner and outer bushings **160**, **170** to the strands **135**. The braid may then be inverted (e.g., by reversing the braiding direction) so that when the medical device **100** is formed, the first end feature **140** is recessed from the proximal end **110** of the device, as shown, and is internal to the medical device.

With reference to FIG. 10, the first end feature **140** may comprise a marker band **172** on an external surface of the outer bushing **170** that is configured to facilitate placement of the medical device **100** at the target site. For example, the marker band **172** may include a radiopaque material, such as a platinum iridium alloy, to allow a medical practitioner to view the location of the medical device **100** (and, more particularly, the location of the proximal end **110** of the medical device) within the body using radio fluoroscopy to facilitate proper delivery and positioning of the device. In some cases, however, the outer bushing **170** itself is made of a radiopaque material, such that the bushing serves as the marker band.

Referring again to FIGS. 4, 6, 7, and 10, the tubular structure **130** may comprise an expanded volume portion

180 proximate the first end feature and a tapered transition portion **190** extending between the expanded volume portion **180** and the proximal end **142** of the first end feature **140**. For example, the inversion of the braid at the proximal end **142** of the first end feature **140** (FIG. 8) may serve to create the tapered transition portion **190**. In the expanded state (e.g., shown in FIG. 2), the expanded volume portion **180** of the tubular structure may have an expanded volume diameter D_e , and the tapered transition portion **190** may define a first transition diameter D_1 proximate the expanded volume portion and a second transition diameter D_2 proximate the proximal end **142** of the first end feature **140**. As shown, the first transition diameter D_1 may be greater than the second transition diameter D_2 , but smaller than the expanded volume diameter D_e . Moreover, the first transition diameter D_1 may be disposed between the second transition diameter D_2 and the expanded volume diameter D_e , and the second transition diameter D_2 may be substantially equal to a diameter of the first end feature **140**.

The tapered transition portion **190** may be configured such that the second transition diameter D_2 is sized to allow tissue growth over the proximal end **110** of the medical device **100**, as shown in FIG. 3. Said differently, because the proximal end **142** of the first end feature **140** substantially coincides with the proximal end **110** of the medical device **100**, the proximal end **110** of the medical device has a small smooth surface (e.g., as compared to the protruding end clamp **20** of the conventional medical device **10** shown in FIG. 1) that allows and facilitates rapid tissue growth over the surface to minimize the chance of a thrombotic embolus being released from the device. For example, as shown in FIG. 10A, the first end feature **140** may include a proximal end surface **145**, a distal end surface (not visible), and a circumferential surface **146** extending between the proximal and distal surfaces. Because of the way the proximal strand ends are secured to the first end feature (as depicted in the figures), the transition portion **190** substantially surrounds the circumferential surface, such that only the proximal end surface (or a portion of the proximal end surface) of the first end feature **140** is exposed to fluid flow through the body lumen.

With reference to FIGS. 6 and 7, the medical device **100** may further comprise a second end feature **150** that is configured to receive and secure distal strand ends **138** (FIG. 6) of the plurality of braided strands. The second end feature **150** may, for example, define a proximal end **152** and a distal end **154**, and the proximal end **152** of the second end feature **150** may define an opening at least partially therethrough. The opening at the proximal end **152** of the second feature **150** may be configured to receive the distal strand ends **138** and may secure them together and/or to the second end feature **150**. For example, the second end feature **150** may be configured to hold the distal strand ends together **138** by clamping, welding, soldering, brazing, or otherwise adhering them to each other and/or to the second end feature **150**. The second end feature **150** may also include a marker band **173** (FIG. 10) to help locate the distal end **120** of the medical device **100**, as noted above with respect to the first end feature **140**. Views of the proximal and distal ends **110**, **120** of the medical device are shown in FIGS. 11 and 12.

In some embodiments, however, not shown, the second end feature **150** may be configured similarly to the first end feature **140**, in that the second end feature **150** may be configured to receive and secure the distal strand ends **138** via the distal end **154** of the second end feature. Thus, the distal end **154** of the second end feature **150** may substantially coincide with the distal end **120** of the medical device

100, which may allow tissue to grow over the surface of the distal end **120** without creating thrombus as noted above with respect to the first end feature **140**. Such a configuration for both the first and second end features **140**, **150** may be especially useful in cases in which both the proximal and distal ends **110**, **120** of the medical device **100** are to be exposed to transverse blood flow.

The medical device **100** may have various configurations depending on factors such as the type of abnormality to be occluded, the location of the target site, the condition of the patient's vasculature, and the practitioner's preferences. For example, in the depicted embodiment of FIG. 7, the medical device **100** has an expanded volume portion **180** proximate the first end feature that defines at least one surface (in this case, two surfaces **182**, **184**) that are substantially perpendicular to a central axis A extending between the first end feature **140** and the second end feature **150**. Moreover, the expanded volume portion **180** may be a first expanded volume portion, and a second expanded volume portion **185** may be provided proximate the second end feature **150** that is displaced axially from the first expanded volume portion **180**. In some cases, as noted above, the tapered transition portion **190** may be a first transition portion, and a second transition portion may be defined that extends between the second expanded volume portion **185** and the second end feature **150** (not shown).

As depicted in FIG. 7, the expanded volume portion **180** may be generally disk shaped, for example, to facilitate maintaining the medical device **100** in position at the target site, as described in greater detail below. The second expanded volume portion **185** may, in some cases, be a generally cylindrically shaped portion that is axially disposed toward the second end feature **150** (e.g., distally from the first end feature **140** and/or the first expanded volume portion **180**). In some cases, the second expanded volume portion **185** may be sized to be somewhat larger in diameter (e.g., about 10-30%), than the inside diameter of the vessel, cavity, or lumen to be occluded. This sizing may be intended to facilitate anchoring the device to prevent dislodgement.

At the same time, the first expanded volume portion **180** of the device **100** may have a diameter that is intended to abut the adjacent wall surrounding the abnormal aperture to prevent device movement toward the second expanded volume portion **185** and to assist in sealing the aperture. For example, the first expanded volume portion **180** may be oversized so as to be capable of overlying the ostium or opening of the LAA and lying adjacent to, and in flush contact with, the wall of the atrium. The diameter of the second expanded volume portion may be less than the diameter of the first volume portion so as to fit in the LAA. The first expanded volume portion **180** may also be flexible so as to be capable of conforming to the curvature of the wall of the atrium in LAA applications or other vascular structures in other applications. Although one configuration of the first and second expanded volume portions **180**, **185** is described above and shown in the figures, various other configurations and sizes may be used depending on the particular application or condition to be treated. For example, one or both expanded volume portions **180**, **185** may be flat disks or disks having a convex distal end, or the device may include a smaller diameter central cylindrical portion between two larger diameter disks. Moreover, the depth or thickness of the first and/or second expanded volume portions may depend on the thickness and number of layers used to make the medical device **100**.

In some embodiments, the tubular structure **130** may further include a flexible connecting portion **188** that

extends between and connects the first expanded volume portion **180** and the second expanded volume portion **185**. The flexible connecting portion **188** may define, for example a narrower connecting diameter D_3 (FIG. 2) with respect to the diameters of the first and second expanded volume portions **180**, **185**, such that the first expanded volume portion **180** is allowed to articulate (e.g., pivot) relative to the second expanded volume portion **185**. In this way, the relative positions of the first and second expanded volume portions **180**, **185** may be adjustable to accommodate different target sites and configurations (e.g., size and location) of abnormal openings to be occluded. Furthermore, the second expanded volume portion **185** may define a conical surface **189** from which the flexible connecting portion **188** extends, as shown in FIG. 7. The conical surface may allow the distance between the first expanded volume portion **180** and the second expanded volume portion **185** to vary and may thus provide a way of creating tension between the expanded volume portions and retention hooks (described below) to maintain the first expanded volume portion **180** over the ostium and keep the device in place.

Referring now to FIGS. 2 and 4, in some embodiments, the medical device **100** may include retention hooks **200**. The retention hooks **200** may be fabricated from Nitinol wire that is heat set into a hook shape at each end and has a bend **205** (FIG. 2), e.g., a bend of less than about 180 degrees, in the mid length segment of the wire so as to create two interconnected hooks. The hooks **200** may also at least partially extend within the medical device **100** in some cases (not shown). In the depicted embodiments, the hooks **200** are disposed on the second expanded volume portion **185**, and the ends **210** of the hooks **200** extend radially out from the second volume portion and are oriented toward the first expanded volume portion **180**. For example, the hooks **200** may be sutured, woven, fastened, or otherwise attached to the braided fabric forming the second expanded volume portion **185**.

According to one embodiment, the wires of the hooks **200** may be about 0.003-0.007 inches in diameter and 2-10 mm in length and may be flexible enough to be back loaded into a delivery catheter or forward loaded if introduced in a straightened-out configuration. The medical device **100** may have any number of hooks **200**, and in some cases three to twelve pairs of hooks may be provided, such as eight pairs of hooks. The hooks **200** may thus be configured to assist in the retention of the medical device **100** by resisting motion of the device in the vessel in a direction that would cause the hooks to engage the tissue. In other words, the hooks **200** are configured to engage body tissue when the medical device **100** is moved along its axis A in the proximal direction. In the depicted embodiment, the hooks **200** do not have barbs so that the engagement with the tissue is reversible by movement of the medical device **100** in a distal direction. Moreover, in LAA applications, for example, the hooks **200** may be configured to penetrate the wall of the LAA, but would not extend completely through the wall of the LAA. Thus, the hooks **200** may reduce the incidence of effusion by not puncturing through the wall of the LAA.

In some embodiments, the hooks **200** may be integral to the medical device **100**, such as when individual strands of the braided tubular structure **130** are isolated, cut, and a short portion of the wire adjacent the cut formed into an outward projecting hook. Such a configuration may provide for a medical device **100** that has a significantly lower profile as no added material (e.g., no separate hooks) contributes to the collapsed overall diameter D_c (FIG. 5) of the medical device during passage through a delivery catheter. In addition,

through the use of integral hooks **200** there are no added suture materials or suture knots that are needed to attach the hooks to the braided tubular structure, which also translates into a reduced profile of the medical device.

As noted above, the second expanded volume portion **185** may be oversized so that it will engage the lumen of the vessel, body organ, or the like to be occluded. The medical device **100** may then be held in place by the combination of the radial engagement of the second expanded volume portion **185** with the lumen of the vessel, body organ, or the like and the engagement of the hooks **200** with the vessel wall. Over a relatively short period of time, thrombi will form in and on the medical device **100** and occlude the lumen. Although the first and second expanded volume portions **180**, **185** may be various sizes, the first expanded volume portion may be at least about 10% larger in diameter than the second expanded volume portion according to one embodiment.

For example, in the case of a medical device **100** that is implanted within the LAA, the medical device **100** may be positioned such that the first expanded volume portion **180** overlies the ostium of the LAA, while the second expanded volume portion **185** is positioned within the LAA. Thus, the first expanded volume portion **180** may be sized and configured to ensure that the first expanded volume portion **180** is implanted to a predetermined depth within the LAA. The second expanded volume portion **185** may in turn be sized and configured to self expand and engage the wall of the LAA, and the hooks **200** may be configured to penetrate into the wall of the LAA, as explained below. Over time, thrombi will form in and on the first and second expanded volume portions **180**, **185** to occlude the LAA.

In some embodiments, in order to speed up the occlusion of the medical device **100**, the medical device may be at least partially coated with a suitable thrombogenic agent, filled with a fiber (e.g., a polymer fabric), braided with an increased number of strands, or include multiple layers of braided strands. For example, the medical device **100** may include one or more layers of polymer fabric **220** positioned within the first and/or second expanded volume portions **180**, **185**, as shown in FIG. 9. In particular, one or more layers of polymer fabric **220** may be sized and configured to be positioned within each of the first and second expanded volume portions **180**, **185**, such that the polymer fabric extends substantially perpendicularly to the axis A of the medical device **100**. Each piece of polymer fabric **220** may be sutured circumferentially about its periphery and about the inner circumference of the first and second expanded volume portions **180**, **185**, respectively. The polymer fabric **220** may be flexible and may be easily collapsed with the medical device **100** for delivery through a catheter. In this way, the interwoven fiber (which in some embodiments may be polyester) may attach to a clot to retain the clot firmly within the device as it forms the occlusion.

Although the embodiments depicted in FIGS. 2-12 show a medical device having a single layer of braided fabric (e.g., a single tubular structure **130**), in some cases a second plurality of strands may be braided to form a second tubular structure, such that medical device includes an inner and outer layer. Referring FIG. 13, for example, the medical device **100** may include an inner layer **250** and an outer layer **260**. The inner layer **250** may be disposed adjacent to the outer layer **260**, and in some cases the inner layer may have a different shape than the outer layer. The first and second expanded volume portions **180**, **185** and the connecting portion **188** may be integrally formed from the same tubular structure.

In some embodiments, the pick count, or the number of strand crossings per unit length of the layers **250**, **260**, may be set at the same or different predetermined values. For example, the inner layer **250** may define a first pick count, and the outer layer **260** may define a second pick count, where the second pick count is different from the first pick count. Although the first pick count, as braided, may be different from the second pick count, as braided, the first and second pick counts may be selected such that the relationship between the reduction in diameter and the elongation of the inner layer **250** is substantially the same as the relationship between the reduction in diameter and the elongation of the outer layer **260** as the medical device **100** is moved between the expanded and contracted states. For example, a ratio of the decrease in diameter of the inner layer **250** to the increase in length of the inner layer **250** may be substantially the same as a ratio of the decrease in diameter of the outer layer **260** to the increase in length of the outer layer **260**. Thus, adjacent portions of the inner and outer layers **250**, **260** may remain in their relative adjacent positions as the medical device **100** is moved between the expanded and contracted states. In this way, the inner layer **250** and the outer layer **260** of the medical device **100** may cooperatively collapse and expand at generally the same rate, which enhances the stability of the medical device and facilitates its delivery into the vessel lumen and subsequent self-expansion. In the case where the inner and outer layers have different shapes from one another, the pick count of each layer may be selected such that in the elongated, contracted state each layer is substantially the same length.

Furthermore, the helix angle of the strands (e.g., the angle formed between the strand and the longitudinal axis of the braid mandrel as the strand is applied to the mandrel) used to braid the plurality of strands of the inner and outer layers **250**, **260** may be the same or different. The helix angles may be selected such that the plurality of strands of the inner layer **250** is braided at a first helix angle, and the plurality of strands of the outer layer **260** is braided at a second helix angle to ensure that the relationship between the reduction in diameter and the elongation of the inner layer is substantially the same as the relationship between the reduction in diameter and the elongation of the outer layer as the at least one layer is moved between the expanded state and the contracted state. In the case where the inner and outer layers have different shapes from one another, the helix angle of each layer may be selected such that in the elongated, contracted state each layer is substantially the same length.

As noted above, the uniform movement that results between the inner and outer layers **250**, **260** may thus reduce the risk of bunching or gathering of the layers within the medical device **100**, which would otherwise reduce the effectiveness of the medical device by increasing its delivery profile and/or generating gaps between the various layers of material that may cause leaks.

The plurality of strands forming the second tubular structure may be made of the same or different material as the strands forming the first tubular structure, described above. Thus, the strands of the second tubular structure may be comprised of metal or polymer material. For example the second tubular structure may be made of stainless steel, other metallic alloys, highly elastic alloys, and/or shape memory alloys, which are both resilient and can be heat treated to substantially set a desired shape, as noted above with respect to the first tubular structure. In addition, polymeric materials may be combined with other materials in the formation of tubular structures for certain applications. For example, the medical device **100** may include a combination

of polyester strands and stainless steel wire. Thus, in some embodiments, the plurality of braided strands of the inner layer **250** may include Nitinol, and the plurality of braided strands of the outer layer **260** may include a polymer, or vice versa.

A method for making a medical device for placement in a body lumen as described above is summarized in FIG. **14**. The method includes braiding a plurality of strands defining proximal strand ends to form a tubular structure at Block **300** and attaching a first end feature defining a proximal end and a distal end to the proximal strand ends via the proximal end of the first end feature at Block **310**. As described above with reference to the figures, the tubular structure may define a molded and heat set resilient expanded volume portion proximate to the first end feature and a tapered transition portion extending between the expanded volume portion and the proximal end of the first end feature. In the expanded state, the expanded volume portion of the tubular structure may define an expanded volume diameter, and the tapered transition portion may define a first transition diameter proximate the expanded volume portion and a second transition diameter proximate the proximal end of the first end feature. As described above and illustrated in the referenced figures, the first transition diameter may be greater than the second transition diameter, smaller than the expanded volume diameter, and disposed between the second transition diameter and the expanded volume diameter. The second transition diameter may be substantially equal to a diameter of the first end feature. In this way, the first end feature may be substantially surrounded by the tapered transition portion, such that the proximal end of the first end feature substantially coincides with the proximal end of the medical device.

As noted above, a second end feature defining a proximal end and a distal end may be attached to the distal strand ends. Block **320**. In some cases, the second end feature may receive the distal strand ends via the proximal end of the second feature, as shown in the figures, whereas in other cases the second end feature may receive the distal strand ends via the distal end of the second end feature similar to the first end feature, thereby also keeping the second end feature from protruding from the distal end of the medical device. The medical device may be modified and configured in various other ways, such as by attaching retention hooks to the tubular structure (e.g., to the outside of second expanded volume portion) (Block **330**), including a polymer fabric in one or more of the expanded volume portions (Block **340**), and/or coating the device with a thrombogenic agent (Block **350**), as described in greater detail above.

Referring now to FIGS. **15A**, **15B**, **16**, and **17**, a delivery device **400** may be provided for deploying embodiments of the medical device **100** described above. The delivery device **400** may include an inner pusher wire **410** with a distal end **415** defining external threads. The external threads of the pusher wire **410** may be configured to engage corresponding internal threads **164** of the first end feature **140** (shown in FIG. **8**) so as to releasably attach the medical device **100** to the delivery device **400** for delivery to and deployment at the target site, as illustrated in FIG. **17**.

The delivery device **400** may further include an outer member **420** defining a lumen through which the inner pusher wire **410** is slideably received. In other words, the inner pusher wire **410** may be axially moveable within the outer member **420**, such that the inner pusher wire may be moved between the position shown in FIG. **15A** and FIG. **15B**, for example. A distal end of the outer member **420** may include a guide member **430** configured to guide the proximal end **110** of the medical device into a distal end of a

delivery sheath **440**. In some cases, the guide member **430** may be made of a polymer material. The guide member **430** may have a tapered external surface, such that the diameter D_d of the guide member at its distal end is approximately the same as (e.g., slightly less than) the inner diameter of the delivery sheath **440** and the diameter D_p of the guide member at its proximal end is approximately the same as (e.g., slightly greater than) the outer diameter of the outer member **420**. Moreover, as shown in FIG. **17**, the distal diameter D_d of the guide member may approximate the second transition diameter D_2 of the transition portion **190**, such that the taper of the transition portion **190** and the guide member generally correspond to one another. In some cases, as shown, the outer surface of the guide member **430** may include grooves or concavities **431**, which may serve to prevent the taper of the guide member from acting as a plunger that draws air into the delivery sheath **440** from the proximal end as the medical device **100** is advanced toward the distal end **445**. In other words, the concavities **431** may allow fluid to flow through the delivery sheath **440**, such that a positive blood pressure exists in the delivery sheath with respect to the pressure outside the body.

The function of the guide member **430** may be illustrated by the following example. When accessing a tortuous path (e.g., a vessel that includes one or more small radius curves), the pusher wire **410** and/or the outer member **420** may be biased to one side of the delivery sheath **440** once the medical device **100** has been deployed (e.g., is outside the delivery sheath **440**, but still attached to the pusher wire **410**). In some cases, the medical device **100** must be recaptured within the delivery sheath **440**, for example, to reposition the medical device at the target site or to replace the device for one of a different size. As the medical device **100** is moved proximally (closer) to the distal end **445** of the delivery sheath **440** during recapture, the medical device **100** may not be axially aligned with the lumen of the delivery sheath (e.g., as a result of the curvature of the vessel within which the delivery sheath is disposed). The guide member **430**, by virtue of its tapered shape, may thus bring the proximal end **110** of the medical device **100** into closer axial alignment with the lumen of the delivery sheath to allow for easier recapture and to minimize the risk of damaging the medical device during recapture.

Accordingly, in FIG. **18**, a method for delivering a medical device as described above is summarized. The method includes providing a medical device configured as described above in connection with one or more of FIGS. **2-17**. Block **500**. For example, the medical device may include a tubular structure comprising a plurality of braided strands defining proximal strand ends and a first end feature defining a proximal end and a distal end, where the first end feature is configured to receive and secure the proximal strand ends via the proximal end of the first end feature. As described above, the tubular structure may define one or more expanded volume portions and at least one tapered transition portion.

The method of delivery may further include advancing the medical device through the body lumen toward the target site (Block **510**) and deploying the medical device at the target site (Block **520**). In some cases, as described above, the method may further include recapturing the medical device within the delivery sheath (Block **530**), repositioning a distal end of the delivery device (Block **540**), and re-deploying the medical device (Block **550**). Once the medical device is positioned at a desired location, the delivery device may be disengaged from the medical device (e.g., via unthreading the medical device from the pusher wire) and

17

withdrawn from the body lumen, leaving the medical device in place at the target site. Block 560.

The method depicted in FIG. 14 and described above represents only one method for making a medical device for placement in a body lumen. Similarly, the method depicted in FIG. 18 and described above represents only one method for delivering a medical device. In some embodiments, certain ones of the steps described above may be modified or further amplified. Furthermore, in some embodiments, additional optional steps may be included, some examples of which are shown in dashed lines in FIGS. 14 and 18. Modifications, additions, or amplifications to the steps above may be performed in any order and in any combination. The particular methods of manufacturing and delivery will depend on the desired configuration of the medical device, the patient's anatomy, the condition and location of the target site, the preferences of the practitioner, and/or other considerations.

This invention has been described herein in considerable detail in order to comply with the Patent Statutes and to provide those skilled in the art with the information needed to apply the novel principles and to construct and use embodiments of the example as required. However, it is to be understood that specifically different devices can carry out the invention and that various modifications can be accomplished without departing from the scope of the invention itself. For example, options shown for one embodiment could easily be applied to other embodiments, as desired for a particular application, without departing from the scope of this invention.

That which is claimed:

1. A medical device configured to self-expand from a contracted state toward an expanded state when deployed from a delivery device, the medical device comprising:

a tubular structure comprising a plurality of braided strands, each braided strand comprising a proximal strand end and a distal strand end; and

18

a first end feature having a proximal end and a distal end, wherein the proximal strand ends are secured to the first end feature such that the proximal strand ends are at least partially inverted at the proximal end of the first end feature.

2. The medical device of claim 1, wherein the tubular structure comprises an expanded volume portion proximate to the first end feature and a tapered transition portion extending between the expanded volume portion and the proximal end of the first end feature.

3. The medical device of claim 2, wherein the first end feature comprises:

a proximal end surface, a distal end surface, and a circumferential surface extending between the proximal and distal end surfaces,

wherein the proximal strand ends are secured to the first end feature such that the tapered transition portion substantially surrounds the circumferential surface of the first end feature and only the proximal end surface of the first end feature or a portion of the proximal end surface is exposed.

4. The medical device of claim 1, wherein the first end feature comprises:

an inner bushing; and

an outer bushing disposed around the inner bushing, wherein the proximal strand ends are secured between the inner bushing and the outer bushing.

5. The medical device of claim 4, wherein the inner bushing and the outer bushing are fused to the proximal strand ends.

6. The medical device of claim 4, wherein the inner bushing comprises threads on an inner surface of the inner bushing for receiving threads of a delivery system.

7. The medical device of claim 4, wherein the first end feature is proximate to a proximal end of the medical device.

* * * * *