

US010772642B2

(12) United States Patent

Kappus et al.

(54) SURGICAL FORCEPS

(71) Applicant: COVIDIEN LP, Mansfield, MA (US)

(72) Inventors: John J. Kappus, Denver, CO (US);

David N. Heard, Boulder, CO (US); Joe D. Sartor, Longmont, CO (US)

(73) Assignee: **COVIDIEN LP**, Mansfield, MA (US)

(*) Notice: Subject to any disclaimer, the term of this

patent is extended or adjusted under 35

U.S.C. 154(b) by 396 days.

(21) Appl. No.: 15/672,383

(22) Filed: Aug. 9, 2017

(65) Prior Publication Data

US 2018/0049752 A1 Feb. 22, 2018

Related U.S. Application Data

- (60) Provisional application No. 62/376,434, filed on Aug. 18, 2016.
- (51) Int. Cl.

 A61B 17/00 (2006.01)

 A61B 17/16 (2006.01)

 (Continued)
- (58) Field of Classification Search
 CPC A61B 17/28; A61B 17/29; A61B 17/1606;
 A61B 17/07207; A61B 17/320016;
 (Continued)

(10) Patent No.: US 10,772,642 B2

(45) **Date of Patent:** Sep. 15, 2020

(56) References Cited

U.S. PATENT DOCUMENTS

D249,549 S 9/1978 Pike D263,020 S 2/1982 Rau, III (Continued)

FOREIGN PATENT DOCUMENTS

CN 201299462 Y 9/2009 DE 2415263 A1 10/1975 (Continued)

OTHER PUBLICATIONS

Heniford et al. "Initial Research and Clinical Results with an Electrothermal Bipolar Vessel Sealer" Oct. 1999.

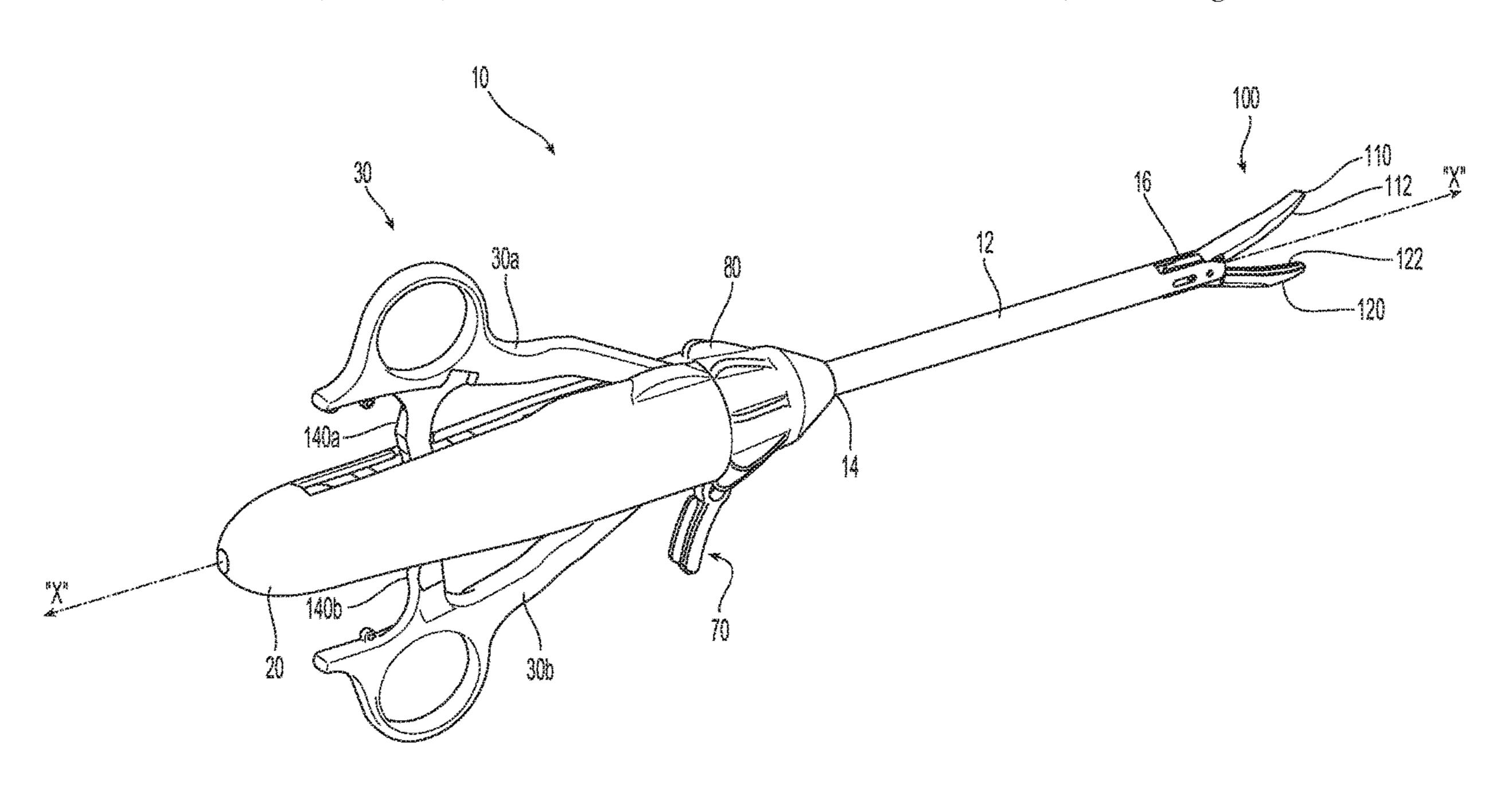
(Continued)

Primary Examiner — Andrew M Tecco
Assistant Examiner — Eyamindae C Jallow
(74) Attorney, Agent, or Firm — Carter, DeLuca & Farrell
LLP

(57) ABSTRACT

A surgical instrument includes a housing, an elongated shaft extending distally from the housing, an end effector assembly, and a trigger assembly. The trigger assembly is disposed in mechanical cooperation with the housing and is configured to longitudinally translate a drive member. The trigger assembly includes a trigger, a gear assembly, a spool, a slider, and a flexible drive member. The trigger is disposed in mechanical cooperation with the gear assembly. The flexible drive member is configured to engage the gear assembly, the spool, and the slider. Movement of the trigger with respect to the housing results in movement of the flexible drive member with respect to the housing and longitudinal movement of the slider with respect to the housing.

19 Claims, 18 Drawing Sheets



(51)	Int. Cl.		D617,901	S	6/2010	Unger et al.
()	A61B 17/29	(2006.01)	D617,902			Twomey et al.
		(2006.01)	D617,903			Unger et al.
	A61B 17/32	(2006.01)	D618,798			Olson et al.
	A61B 17/295	(2006.01)	D621,503			Otten et al.
			D627,462			Kingsley
	A61B 18/14	(2006.01)	· · · · · · · · · · · · · · · · · · ·			
	A61B 17/3201	(2006.01)	D628,289			Romero
	A61B 34/30	(2016.01)	D628,290			Romero
			D630,324			Reschke
	A61B 90/00	(2016.01)	D649,249		11/2011	
(52)	U.S. Cl.		D649,643	S	11/2011	Allen, IV et al.
(32)		0017 (0010 01). AZID 10/1445	D661,394	S	6/2012	Romero et al.
		0016 (2013.01); A61B 18/1445	D670,808	S	11/2012	Moua et al.
	(2013.01); A	161B 17/3201 (2013.01); A61B	D680,220	S	4/2013	Rachlin
	34/30 (2016 02)	; A61B 90/03 (2016.02); A61B	9,084,608	B2	7/2015	Larson et al.
		, , , , , , , , , , , , , , , , , , , ,	9,211,657			Ackley et al.
		53 (2013.01); A61B 2017/2913	9,566,065			Knodel A61B 17/068
	(2013.01); A61	<i>B 2017/2915</i> (2013.01); <i>A61B</i>	2005/0209596			Daniels et al.
	2017/292	23 (2013.01); A61B 2018/1452	2007/0175964			Shelton, IV A61B 17/072
	20177272		2007/0173304	Λ 1	0/2007	
		(2013.01)	2010/0004655	A 1	1/2010	227/180.1
(58)	Field of Classification	n Search	2010/0004677			Brostoff et al.
	CPC A61B 2017/0	0353; A61B 2017/2923; A61B	2011/02/6049	Al*	11/2011	Gerhardt A61B 18/1402
	C1 C 1101D 201770					606/45
	<i>a</i>	2017/2943	2012/0316601	A 1	12/2012	Twomey
	See application file for	or complete search history.	2014/0221995	A 1	8/2014	Guerra et al.
			2014/0221999			Cunningham et al.
(56)	Referen	ces Cited	2014/0228842			Dycus et al.
(20)	IXCICICI		2014/0230243			Roy et al.
	TIC DATENTE	DOCIMENTS	2014/0236149			Kharin et al.
	U.S. PATENT	DOCUMENTS	2014/0243811			Reschke et al.
			2014/0243824			Gilbert
		Sharkany et al.				
	D295,894 S 5/1988	Sharkany et al.	2014/0249528			Hixson et al.
	D298,353 S 11/1988	Manno	2014/0250686			Hempstead et al.
	D299,413 S 1/1989	DeCarolis	2014/0257274			McCullough, Jr. et al.
	D343,453 S 1/1994	Noda	2014/0257283			Johnson et al.
	D348,930 S 7/1994	Olson	2014/0257284		9/2014	
	*	Lichtman et al.	2014/0257285	$\mathbf{A}1$	9/2014	Moua
	,	Medema	2014/0276803		9/2014	Hart
	D358,887 S 5/1995		2014/0284313	A 1	9/2014	Allen, IV et al.
	·	Foshee A61B 17/2909	2014/0288549	$\mathbf{A}1$	9/2014	McKenna et al.
	5,562,015 A 12/1550		2014/0288553	A 1	9/2014	Johnson et al.
	D204 412 C 0/1007	7114 -1	2014/0330308	A1	11/2014	Hart et al.
	,	Zlock et al.	2014/0332578	A1*	11/2014	Fernandez A61B 17/068
		Paraschac				227/175.1
	· · · · · · · · · · · · · · · · · · ·	Grimm et al.	2014/0336635	Δ1	11/2014	Hart et al.
	·	McNaughton		_		Motooka A61B 17/07207
	, , , , , , , , , , , , , , , , , , ,	Barton et al.	2017/0337200	$\Lambda 1$	11/2017	
		Tetzlaff et al.	2014/0252199	A 1	10/2014	December 227/175.2
	D425,201 S 5/2000	Tetzlaff et al.	2014/0353188			Reschke et al.
	H1904 H 10/2000	Yates et al.	2015/0018816			Latimer
	D449,886 S 10/2001	Tetzlaff et al.	2015/0025528		1/2015	
	D453,923 S 2/2002	Olson	2015/0032106			Rachlin
	D454,951 S 3/2002	Bon	2015/0051598			Orszulak et al.
	D457,958 S 5/2002	Dycus et al.	2015/0051640			Twomey et al.
	•	Tetzlaff et al.	2015/0066026	Al	3/2015	Hart et al.
	,	Yates et al.	2015/0080880	A1	3/2015	Sartor et al.
	D465,281 S 11/2002		2015/0080889	A1	3/2015	Cunningham et al.
	D466,209 S 11/2002		2015/0082928			Kappus et al.
	D493,888 S 8/2004		2015/0088122			Jensen
	· ·	Dycus et al.	2015/0088126			Duffin et al.
		Dycus et al. Dycus et al.				
	,	Blake, III	2015/0088128			Couture
			2015/0094714			Lee et al.
	D509,297 S 9/2005		2015/0209059	A1*	7/2015	Trees A61B 18/1445
	D525,361 S 7/2006					606/170
	,	Guerra et al.	2016/0135869	A1*	5/2016	Jadhav F16H 19/06
		Visconti et al.				606/52
	,	Kerr et al.	2017/0143361	A 1 *	5/2017	Boudreaux A61B 17/29
	,	James et al.	2017/0143362			Cagle A61B 18/1445
	D538,932 S 3/2007		ZV17/V1 4 330Z	$\Delta 1$	5/201/	Cagic AUID 16/1443
	, , , , , , , , , , , , , , , , , , ,	Schechter et al.		N TT		
	D541,611 S 5/2007	Aglassinger	FO	KEIGI	N PATE	NT DOCUMENTS
		Kerr et al.				
	,	Watanabe	DE	02514	501 A1	10/1976
	D547,154 S 7/2007		DE		679 A1	1/1977
		Moses et al.	DE		356 C2	6/1986
	· · · · · · · · · · · · · · · · · · ·	Moses et al.	DE		646 A1	4/1987
	,	Hushka	DE		221 A1	2/1988
		Hixson et al.	DE		328 U1	2/1988
		Swoyer et al.	DE		417 A1	10/1993
	•	Kingsley et al.	DE		882 C2	2/1995
	D017,200 B 0/2010	ixingsicy of ai.	1/1/	CUCFO	002 02	2/1/J

(56)	References Cited	SU 401367 A1 10/1973
		WO 0036986 A1 6/2000
	FOREIGN PATENT DOCUMENTS	WO 0059392 A1 10/2000 WO 0115614 A1 3/2001
DE	04403252 A1 8/1995	WO 0113611 711 3/2001 WO 0154604 A1 8/2001
DE	19515914 C1 7/1996	WO 02/45589 A2 6/2002
DE	19506363 A1 8/1996	WO 06/021269 A1 3/2006
DE	29616210 U1 11/1996	WO 05110264 A3 4/2006
DE	19608716 C1 4/1997	WO 08/040483 A1 4/2008 WO 2011/018154 A1 2/2011
DE DE	19751106 A1 5/1998 19738457 A1 3/1999	2011/010154 711 2/2011
DE	19751108 A1 5/1999	
DE	19946527 C1 7/2001	OTHER PUBLICATIONS
DE	10031773 A1 11/2001	Extended European Search Report for EP 16196110 dated Dec. 23,
DE	10045375 A1 4/2002	2016.
DE DE	20121161 U1 4/2002 102004026179 A1 12/2005	
DE DE	202007009165 U1 8/2007	Michael Choti, "Abdominoperineal Resection with the LigaSure Vessel Sealing System and LigaSure Atlas 20 cm Open Instrument";
DE	202007009318 U1 8/2007	Innovations That Work, Jun. 2003.
DE	202007009317 U1 10/2007	Chung et al., "Clinical Experience of Sutureless Closed
DE	202007016233 U1 1/2008	Hemontoidectomy with LigaSure" Diseases of the Colon & Rectum
DE	102008018406 B3 7/2009	vol. 46, No. 1 Jan. 2003.
EP EP	0589453 A2 3/1994 1159926 A2 12/2001	Tinkcler L.F., "Combined Diathermy and Suction Forceps", Feb. 6,
EP	1281878 A1 2/2003	1967 (Feb. 6, 1967), British Medical Journal Feb. 6, 1976, vol. 1,
\mathbf{EP}	2777586 A1 9/2014	nr. 5431 p. 361, ISSN: 0007-1447.
EP	2890309 A1 7/2015	Carbonell et al., "Comparison of theGyrus PlasmaKinetic Sealer
JP	61-501068 9/1984	and the Valleylab LigaSure Device in the Hemostasis of Small,
JP JP	11-47150 A 6/1989 6-502328 3/1992	Medium, and Large-Sized Arteries" Carolinas Laparoscopic and
JP	5-5106 1/1993	Advanced Surgery Program, Carolinas Medical Center, Charlot-
JP	05-40112 2/1993	te,NC; Date: Aug. 2003.
JP	0006030945 A 2/1994	Peterson et al. "Comparison of Healing Process Following Ligation
JP	6-121797 A 5/1994	with Sutures and Bipolar Vessel Sealing" Surgical Technology
JP JP	6-285078 A 10/1994 6-511401 12/1994	International (2001).
JP	06343644 A 12/1994	"Electrosurgery: A Historical Overview" Innovations in Electrosurgery;
JP	07265328 A 10/1995	Sales/Product Literature; Dec. 31, 2000. (6 pages).
JP	8-56955 3/1996	Johnson et al. "Evaluation of a Bipolar Electrothermal Vessel
JP	08252263 A 10/1996	Sealing Device in Hemorrhoidectomy" Sales/Product Literature;
JP JP	8-289895 A 11/1996 8-317934 A 12/1996	Jan. 2004. (1 page).
JP	8-317936 A 12/1996	E. David Crawford "Evaluation of a New Vessel Sealing Device in
JP	910223 1/1997	Urologic Cancer Surgery' Sales/Product Literature 2000.
JP	09000538 A 1/1997	Johnson et al. "Evaluation of the LigaSure Vessel Sealing System in
JP JP	9-122138 A 5/1997 1024051 1/1998	Hemorrhoidectormy" American College of Surgeons (ACS) Clinicla Congress Poster (2000).
JP	0010000195 A 1/1998	Muller et al., "Extended Left Hemicolectomy Using the LigaSure
JP	10-155798 A 6/1998	Vessel Sealing System" Innovations That Work, Sep. 1999.
JP	11-47149 2/1999	Kennedy et al. "High-burst-strength, feedback-controlled bipolar
JP	11-070124 A 3/1999	vessel sealing" Surgical Endoscopy (1998) 12: 876-878.
JP JP	11-169381 A 6/1999 11-192238 A 7/1999	Burdette et al. "In Vivo Probe Measurement Technique for Deter-
JP	11244298 A 9/1999	mining Dielectric Properties at VHF Through Microwave Frequen-
JP	2000-102545 A 4/2000	cies", IEEE Transactions on Microwave Theory and Techniques,
JP	2000-135222 A 5/2000	vol. MTT-28, No. 4, Apr. 1980 pp. 414-427.
JP	2000342599 A 12/2000	Carus et al., "Initial Experience With the LigaSure Vessel Sealing
JP JP	2000350732 A 12/2000 2001008944 A 1/2001	System in Abdominal Surgery' Innovations That Work, Jun. 2002.
JP	2001-029355 A 2/2001	Heniford et al. "Initial Results with an Electrothermal Bipolar
JP	2001029356 A 2/2001	Vessel Sealer" Surgical Endoscopy (2000) 15:799-801. (4 pages).
JP	2001128990 A 5/2001	Herman et al., "Laparoscopic Intestinal Resection With the LigaSure
JP JP	2001-190564 A 7/2001 2001-003400 11/2001	Vessel Sealing System: A Case Report"; Innovations That Work,
JP	2001-003400 11/2001 2002-136525 A 5/2002	Feb. 2002. Koyle et al., "Laparoscopic Palomo Varicocele Ligation in Children
JP	2002-528166 A 9/2002	and Adolescents" Pediatric Endosurgery & Innovative Techniques,
JP	2003-116871 A 4/2003	vol. 6, No. 1, 2002.
JP	2003-175052 A 6/2003	W. Scott Helton, "LigaSure Vessel Sealing System: Revolutionary
JP ID	2003245285 A 9/2003	Hemostasis Product for General Surgery"; Sales/Product Literature
JP JP	2004-517668 A 6/2004 2004-528869 A 9/2004	1999.
JP	2004-328609 A 9/2004 2005-152663 A 6/2005	LigaSure Vessel Sealing System, the Seal of Confidence in General,
JP	2005-253789 A 9/2005	Gynecologic, Urologic, and Laparaoscopic Surgery; Sales/Product
JP	2005312807 A 11/2005	Literature; Apr. 2002.
JP	2006-015078 A 1/2006	Joseph Ortenberg "LigaSure System Used in Laparoscopic 1st and
JP ID	2006-501939 A 1/2006	2nd Stage Orchiopexy" Innovations That Work, Nov. 2002.
JP JP	2006-095316 A 4/2006 2008-054926 A 3/2008	Sigel et al. "The Mechanism of Blood Vessel Closure by High Frequency Electrocoagulation" Surgery Gynecology & Obstetrics,
JР	2008-034926 A	Oct. 1965 pp. 823-831.
		L L

(56) References Cited

OTHER PUBLICATIONS

Sampayan et al, "Multilayer Ultra-High Gradient Insulator Technology" Discharges and Electrical Insulation in Vacuum, 1998. Netherlands Aug. 17-21, 1998; vol. 2, pp. 740-743.

Paul G. Horgan, "A Novel Technique for Parenchymal Division During Hepatectomy" The American Journal of Surgery, vol. 181, No. 3, Apr. 2001 pp. 236-237.

Benaron et al., "Optical Time-Of-Flight and Absorbance Imaging of Biologic Media", Science, American Association for the Advancement of Science, Washington, DC, vol. 259, Mar. 5, 1993, pp. 1463-1466.

Olsson et al. "Radical Cystectomy in Females" Current Surgical Techniques in Urology, vol. 14, Issue 3, 2001.

Palazzo et al. "Randomized clinical trial of Ligasure versus open haemorrhoidectomy" British Journal of Surgery 2002, 89, 154-157. Levy et al. "Randomized Trial of Suture Versus Electrosurgical Bipolar Vessel Sealing in Vaginal Hysterectomy" Obstetrics & Gynecology, vol. 102, No. 1, Jul. 2003.

"Reducing Needlestick Injuries in the Operating Room" Sales/ Product Literature 2001. (1 page).

Bergdahl et al. "Studies on Coagulation and the Development of an Automatic Computerized Bipolar Coagulator" J. Neurosurg, vol. 75, Jul. 1991, pp. 148-151.

Strasberg et al. "A Phase I Study of the LigaSure Vessel Sealing System in Hepatic Surgery" Section of HPB Surger, Washington University School of Medicine, St. Louis MO, Presented at AHPBA, Feb. 2001.

Sayfan et al. "Sutureless Closed Hemorrhoidectomy: A New Technique" Annals of Surgery vol. 234 No. 1 Jul. 2001; pp. 21-24.

Levy et al., "Update on Hysterectomy—New Technologies and Techniques" OBG Management, Feb. 2003. (15 pages).

Dulemba et al. "Use of a Bipolar Electrothermal Vessel Sealer in Laparoscopically Assisted Vaginal Hysterectomy" Sales/Product Literature; Jan. 2004.

Strasberg et al., "Use of a Bipolar Vessel-Sealing Device for Parenchymal Transection During Liver Surgery" Journal of Gastrointestinal Surgery, vol. 6, No. 4, Jul./Aug. 2002 pp. 569-574. Sengupta et al., "Use of a Computer-Controlled Bipolar Diathermy System in Radical Prostatectomies and Other Open Urological

Surgery" ANZ Journal of Surgery (2001) 71.9 pp. 538-540.

Rothenberg et al. "Use of the LigaSure Vessel Sealing System in Minimally Invasive Surgery in Children" Int'l Pediatric Endosurgery Group (IPEG) 2000.

Crawford et al. "Use of the LigaSure Vessel Sealing System in Urologic Cancer Surgery" Grand Rounds in Urology 1999 vol. 1 Issue 4 pp. 10-17.

Craig Johnson, "Use of the LigaSure Vessel Sealing System in Bloodless Hemorrhoidectomy" Innovations That Work, Mar. 2000. Levy et al. "Use of a New Energy-based Vessel Ligation Device During Vaginal Hysterectomy" Int'l Federation of Gynecology and Obstetrics (FIGO) World Congress 1999.

Barbara Levy, "Use of a New Vessel Ligation Device During Vaginal Hysterectomy" FIGO 2000, Washington, D.C.. (1 page). E. David Crawford "Use of a Novel Vessel Sealing Technology in Management of the Dorsal Veinous Complex" Sales/ Product Literature 2000.

Jarrett et al., "Use of the LigaSure Vessel Sealing System for Peri-Hilar Vessels in Laparoscopic Nephrectomy" Sales/Product Literature 2000.

Crouch et al. "A Velocity-Dependent Model for Needle Insertion in Soft Tissue" MICCAI 2005; LNCS 3750 pp. 624-632, Dated: 2005. McLellan et al. "Vessel Sealing for Hemostasis During Pelvic Surgery" Int'l Federation of Gynecology and Obstetrics FIGO World Congress 2000, Washington, D.C.

McLellan et al. "Vessel Sealing for Hemostasis During Gynecologic Surgery" Sales/Product Literature 1999.

U.S. Appl. No. 08/926,869, filed Sep. 10, 1997; inventor: James G. Chandler, Abandoned.

U.S. Appl. No. 09/177,950, filed Oct. 23, 1998; inventor: Randel A. Frazier, abandoned.

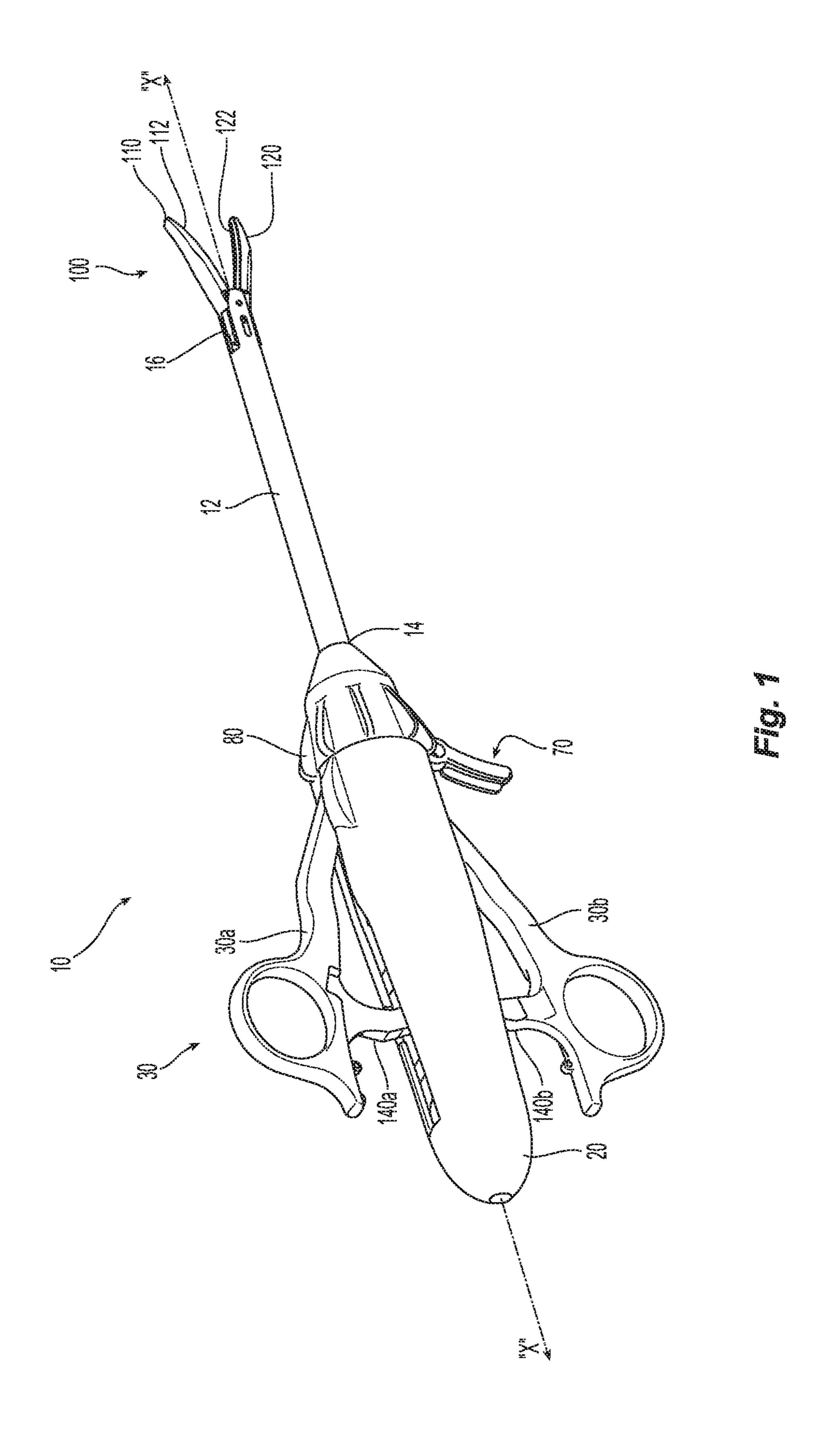
U.S. Appl. No. 09/387,883, filed Sep. 1, 1999; inventor: Dale F. Schmaltz, abandoned.

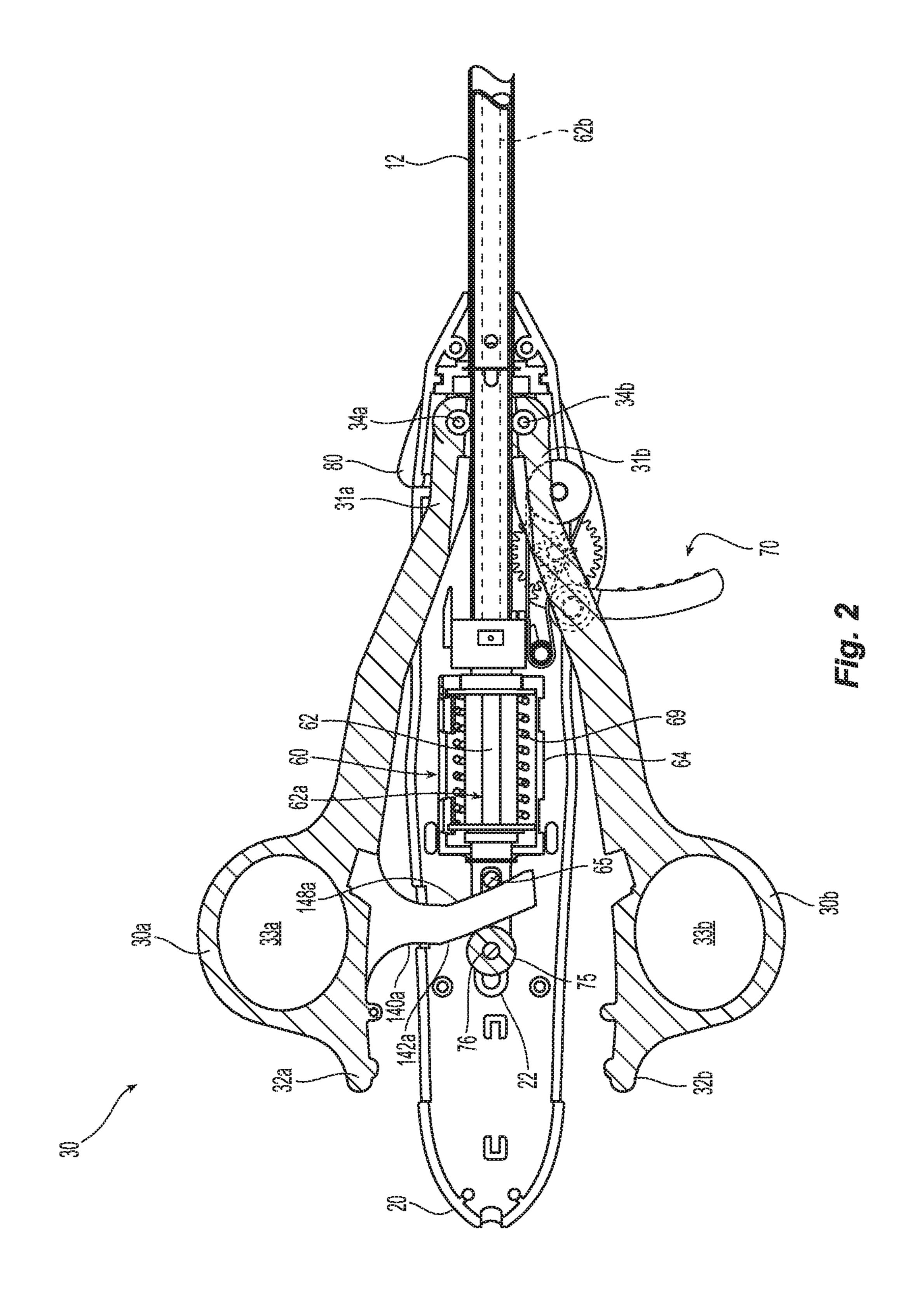
U.S. Appl. No. 09/591,328, filed Jun. 9, 2000; inventor: Thomas P. Ryan, abandoned.

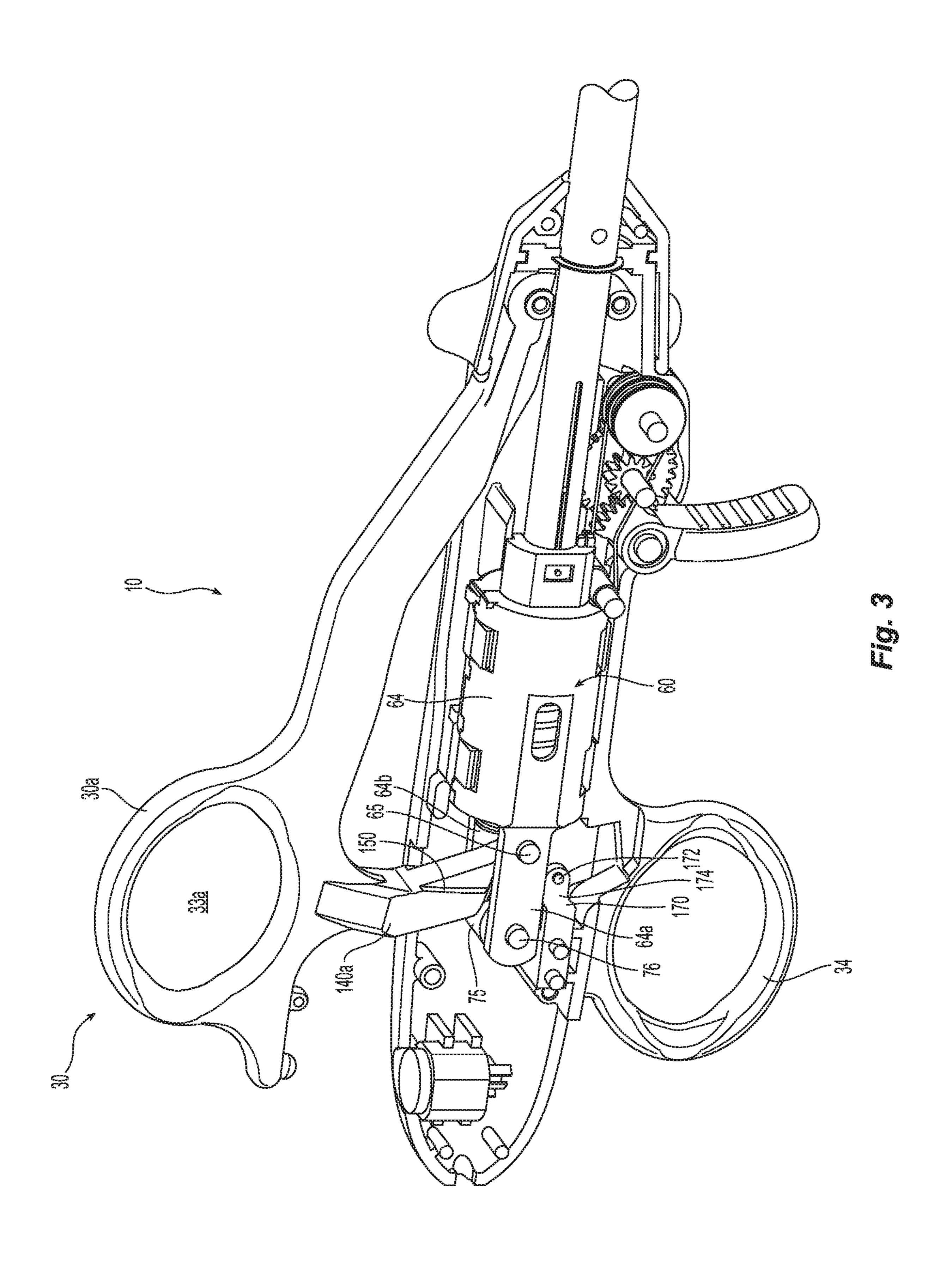
U.S. Appl. No. 12/336,970; filed Dec. 17, 2008; inventor: Paul R. Sremeich, abandoned.

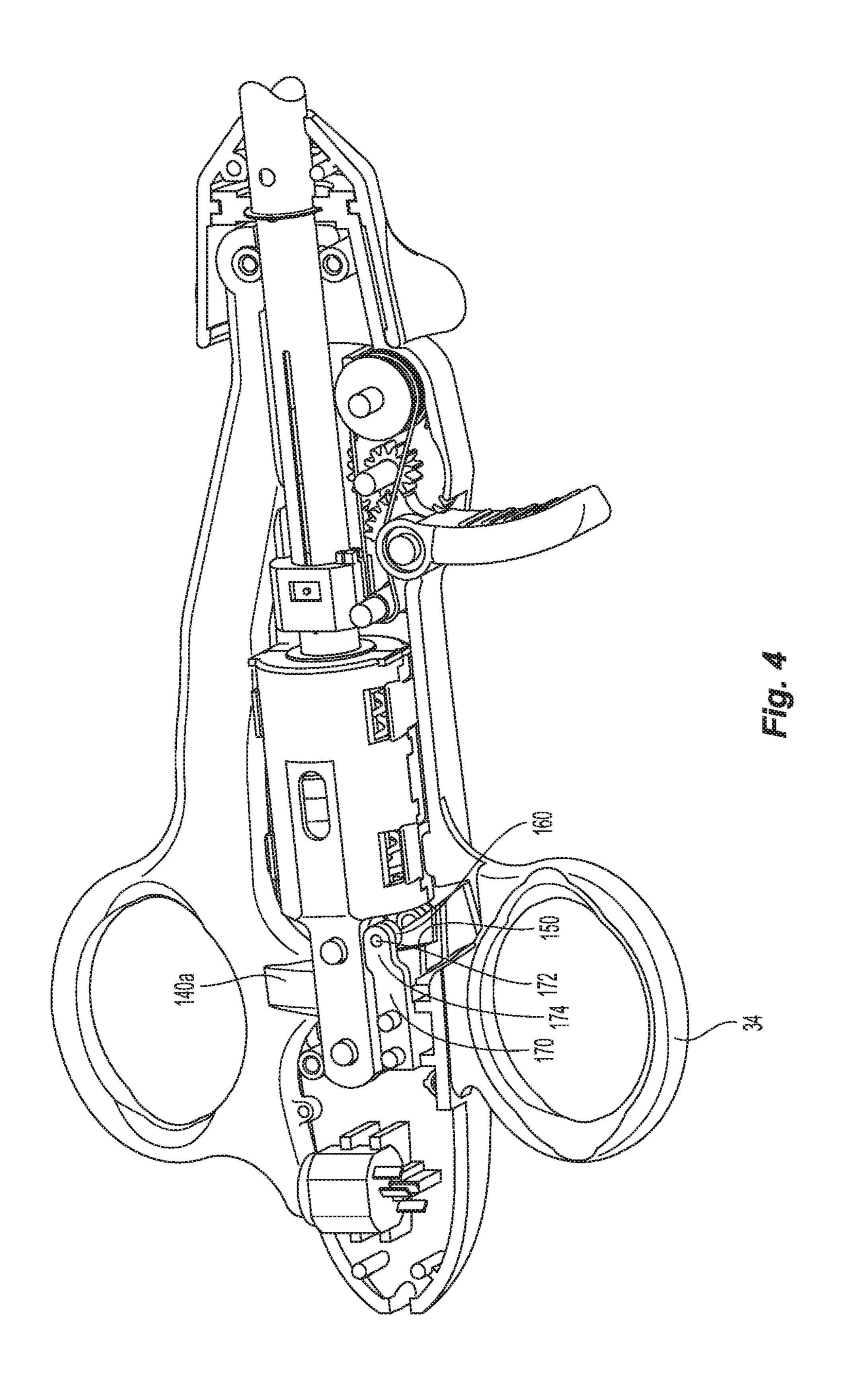
U.S. Appl. No. 14/065,644, filed Oct. 29, 2013; inventor: Reschke, abandoned.

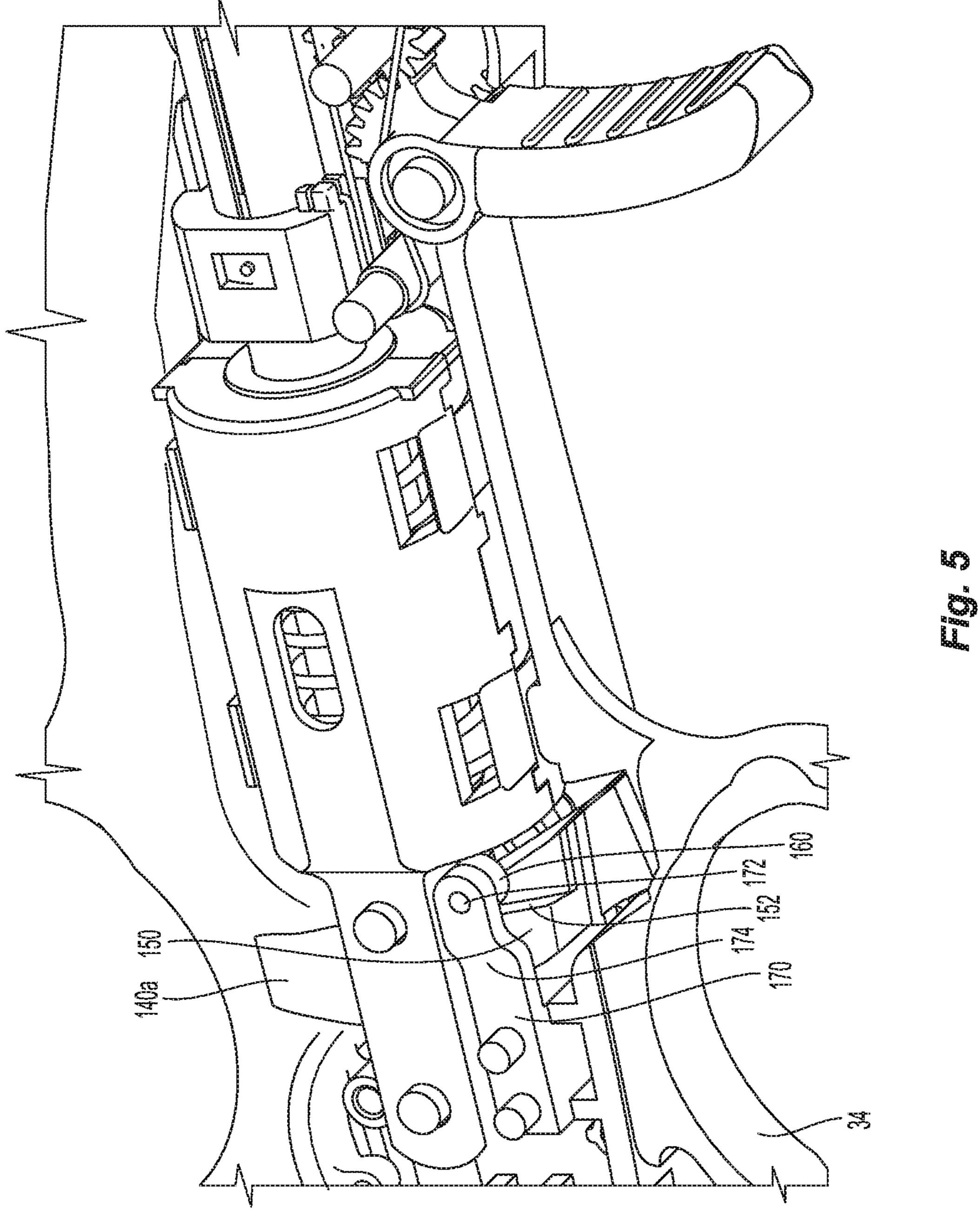
* cited by examiner

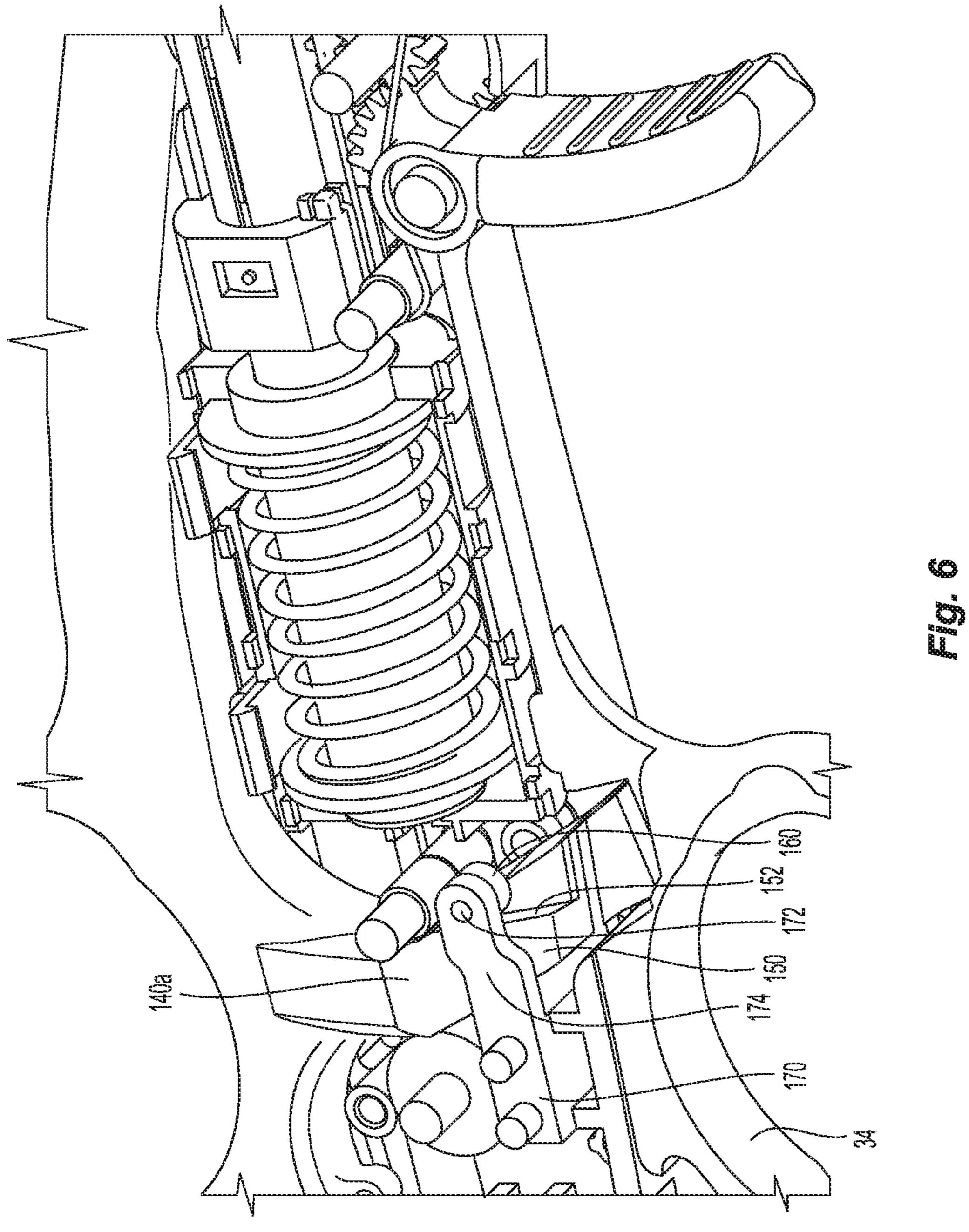


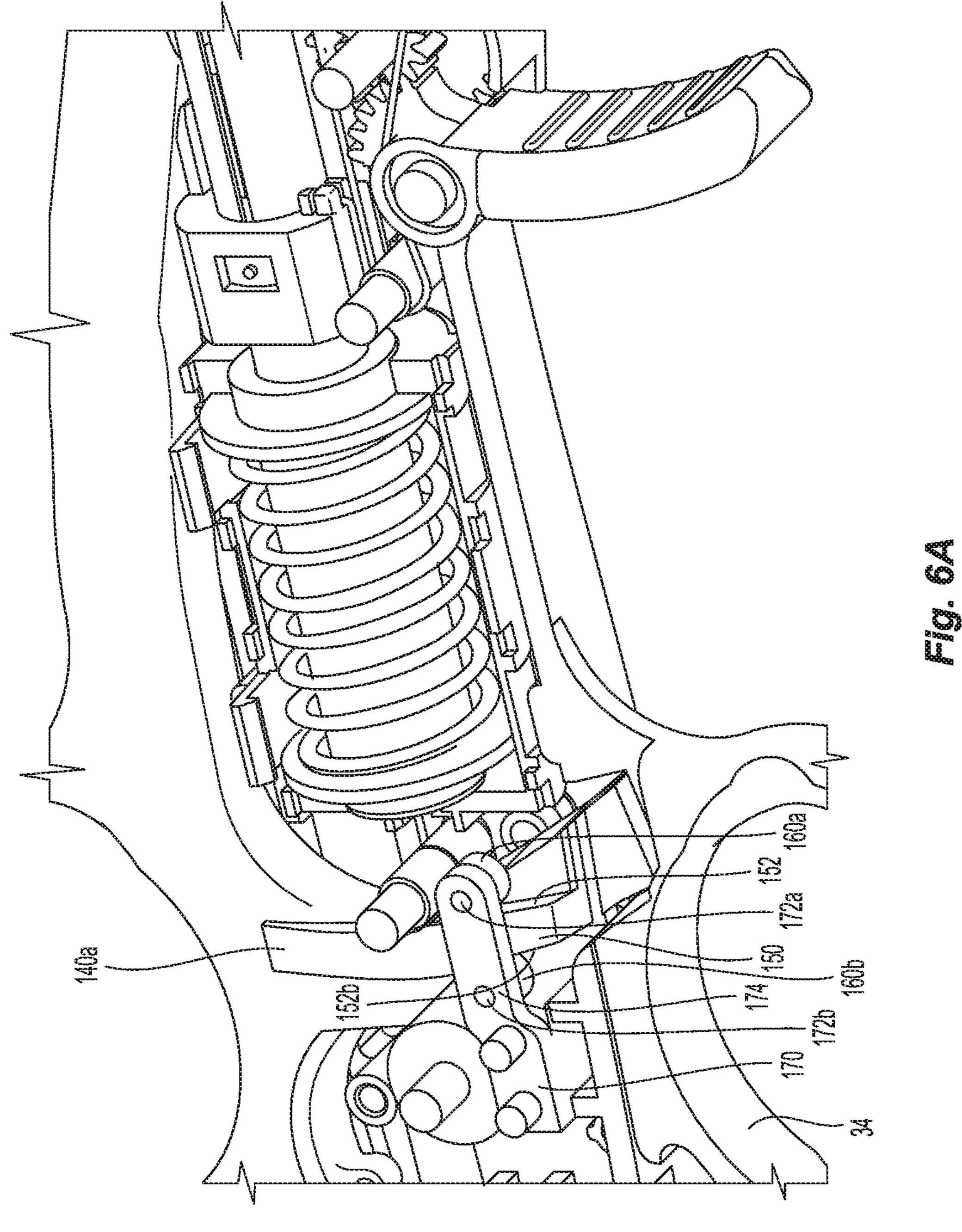


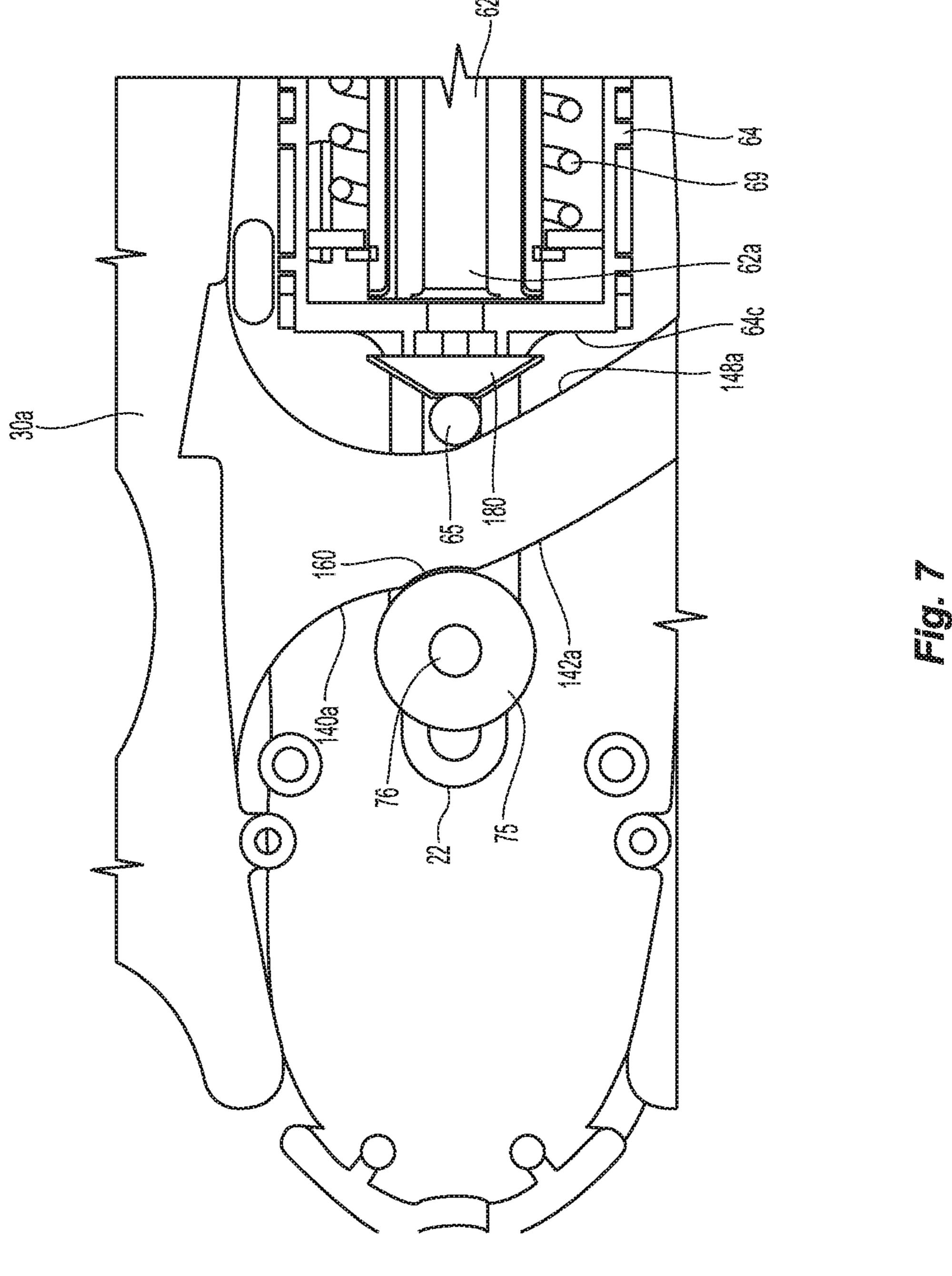


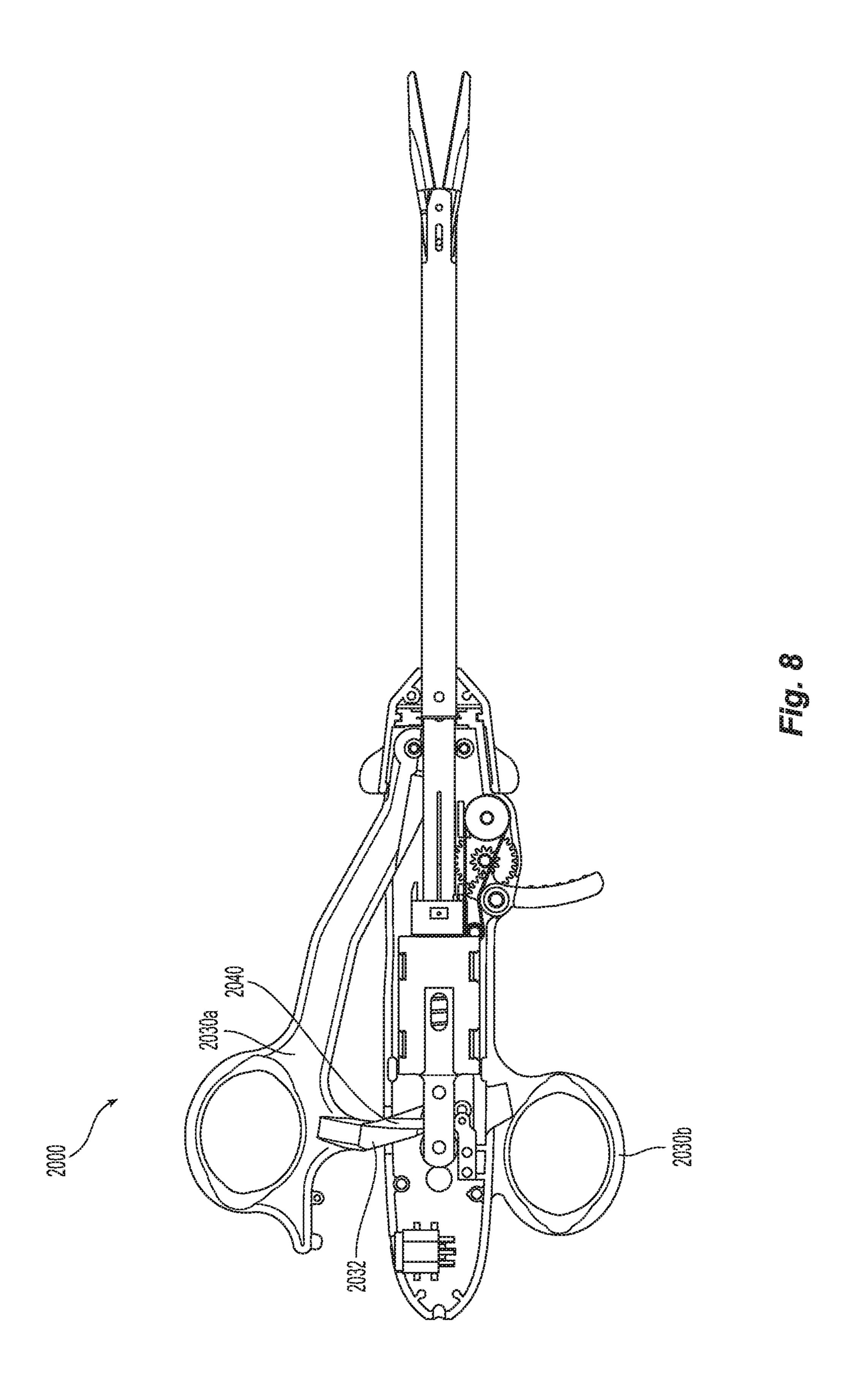


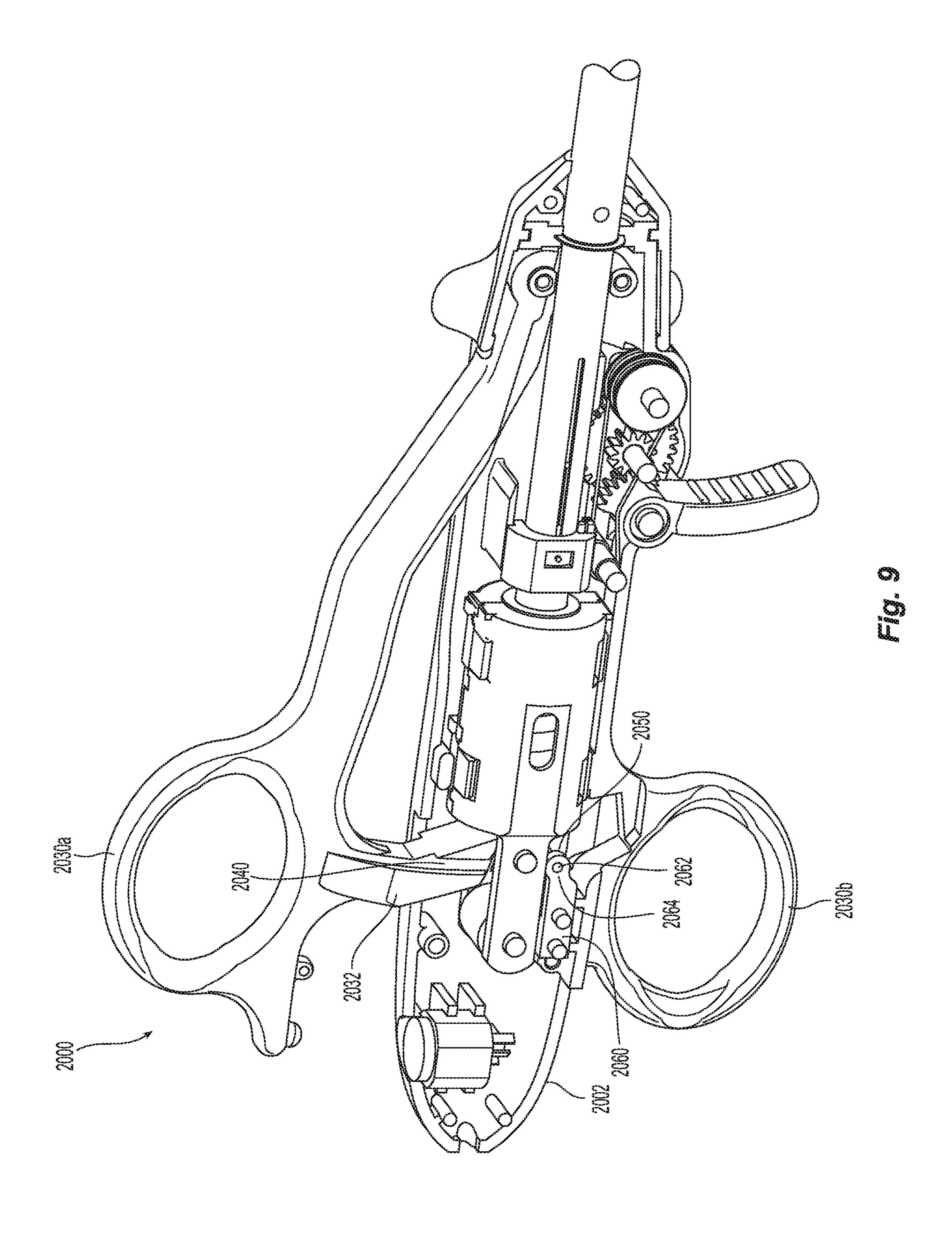


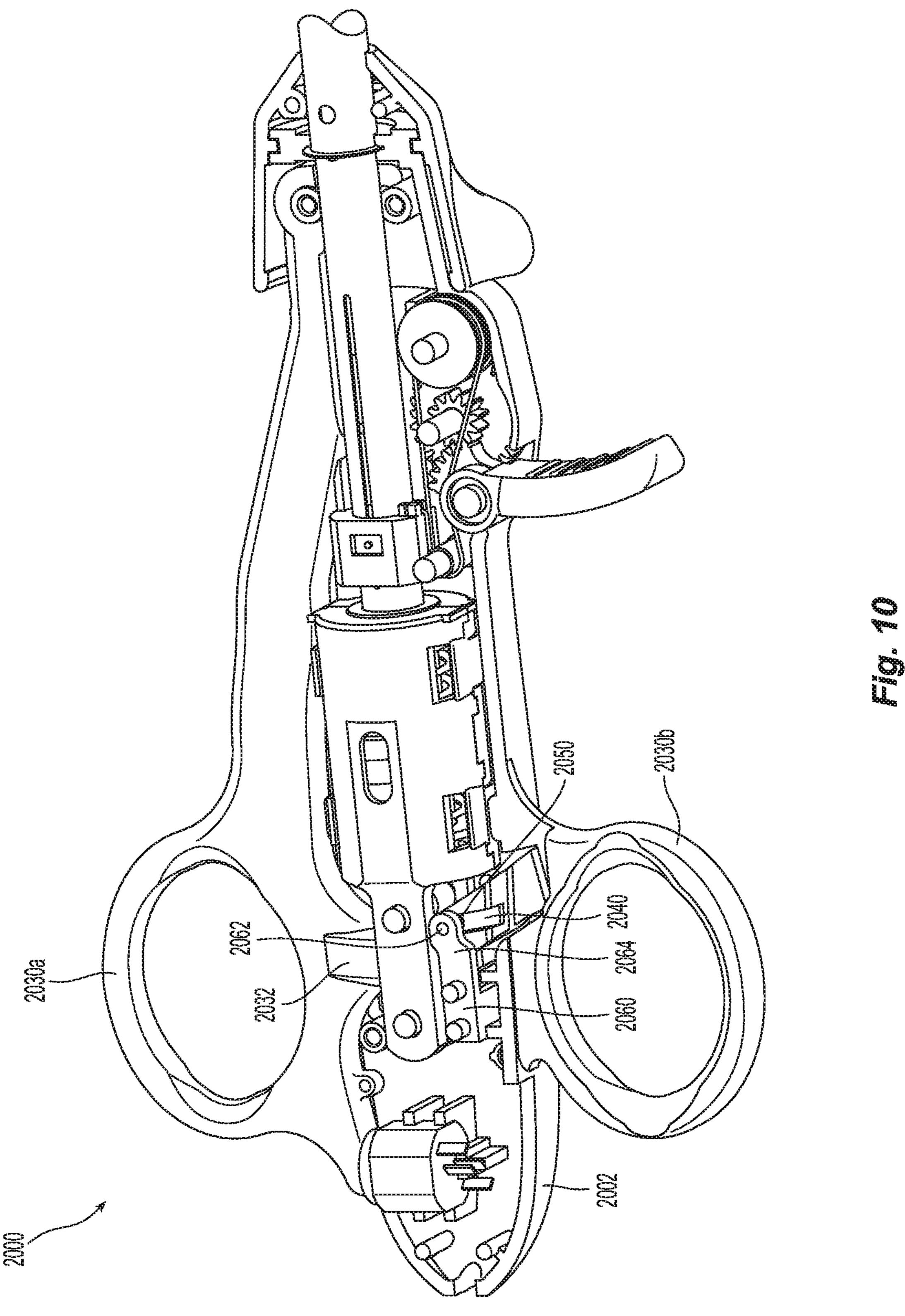


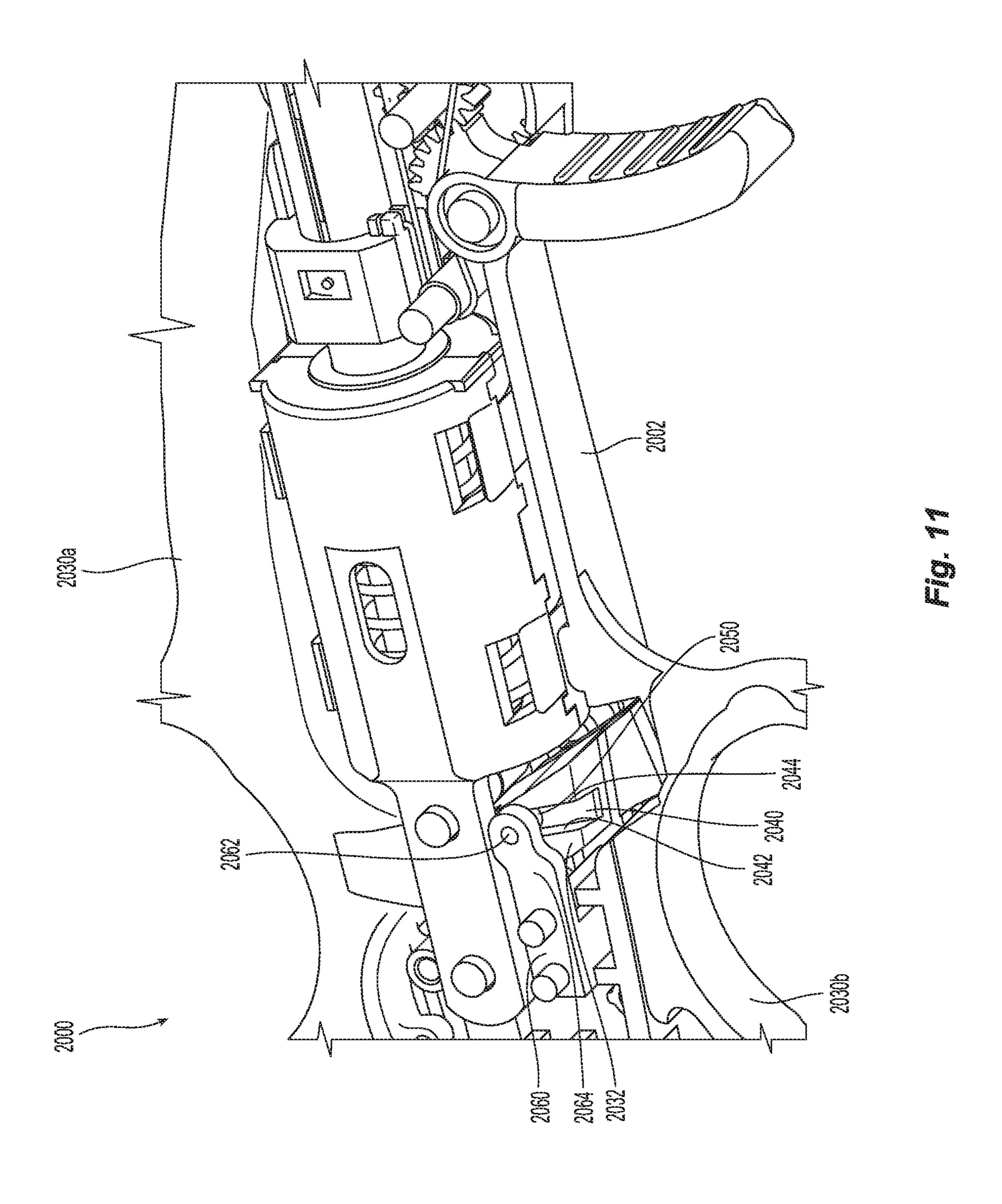


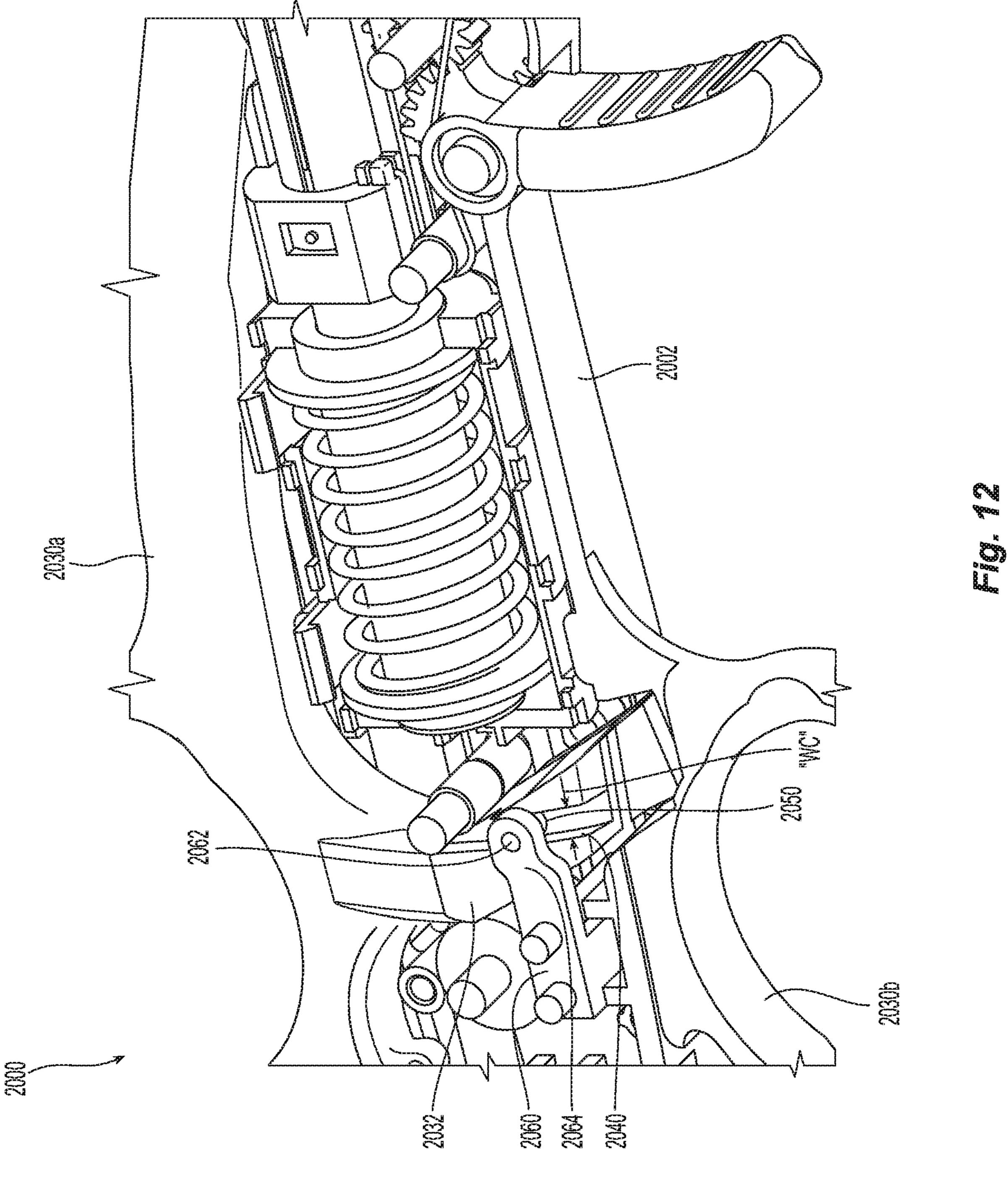


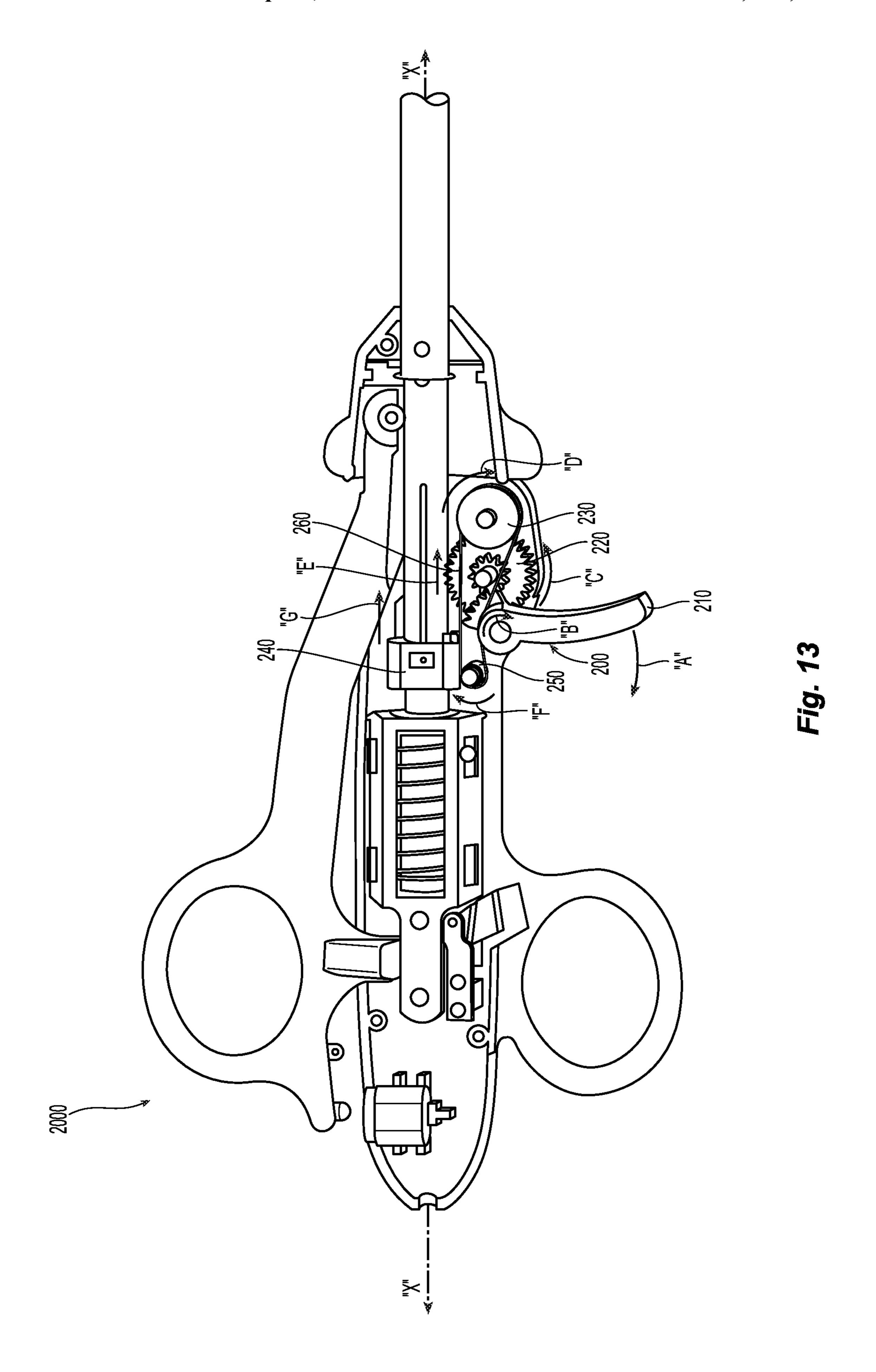


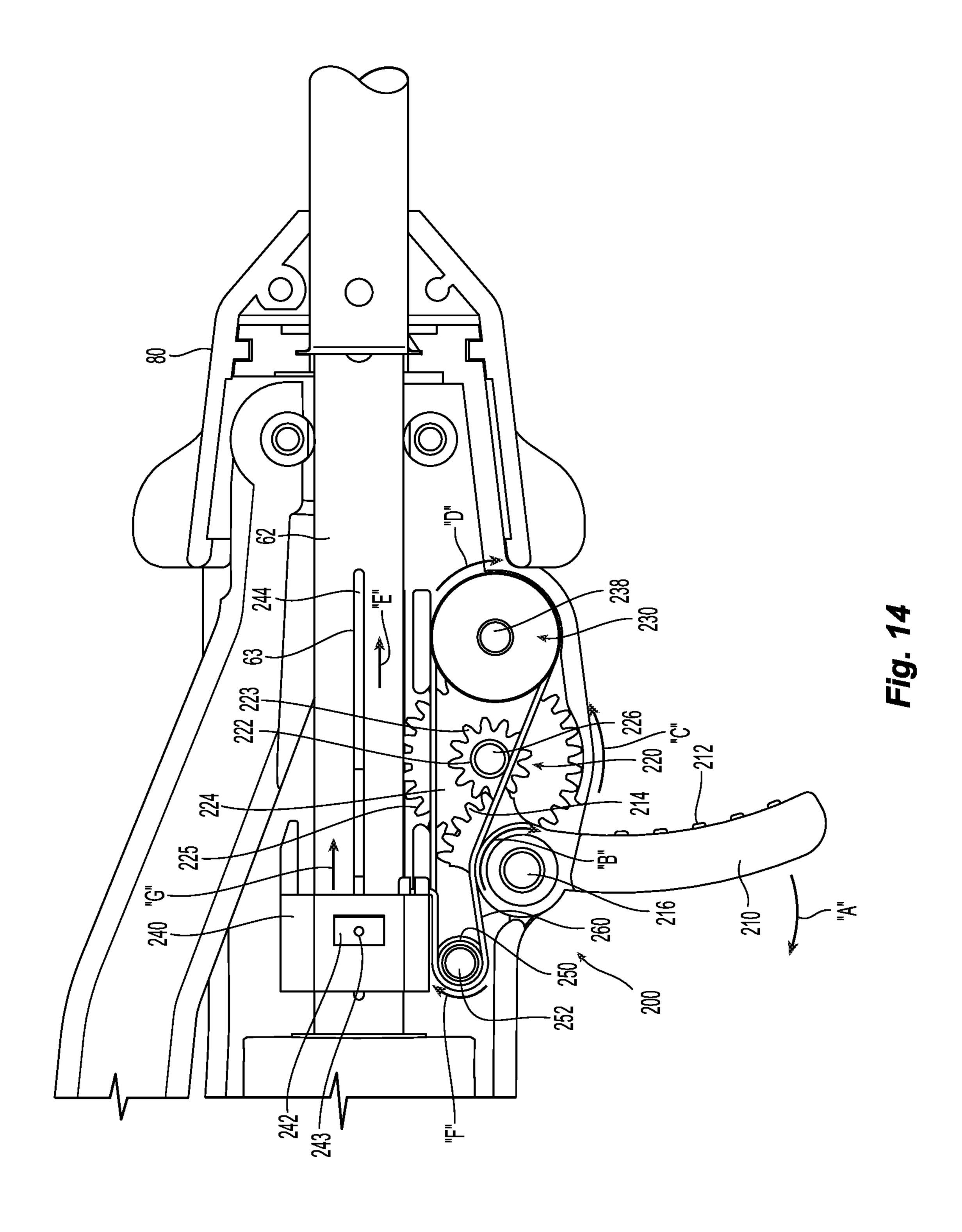


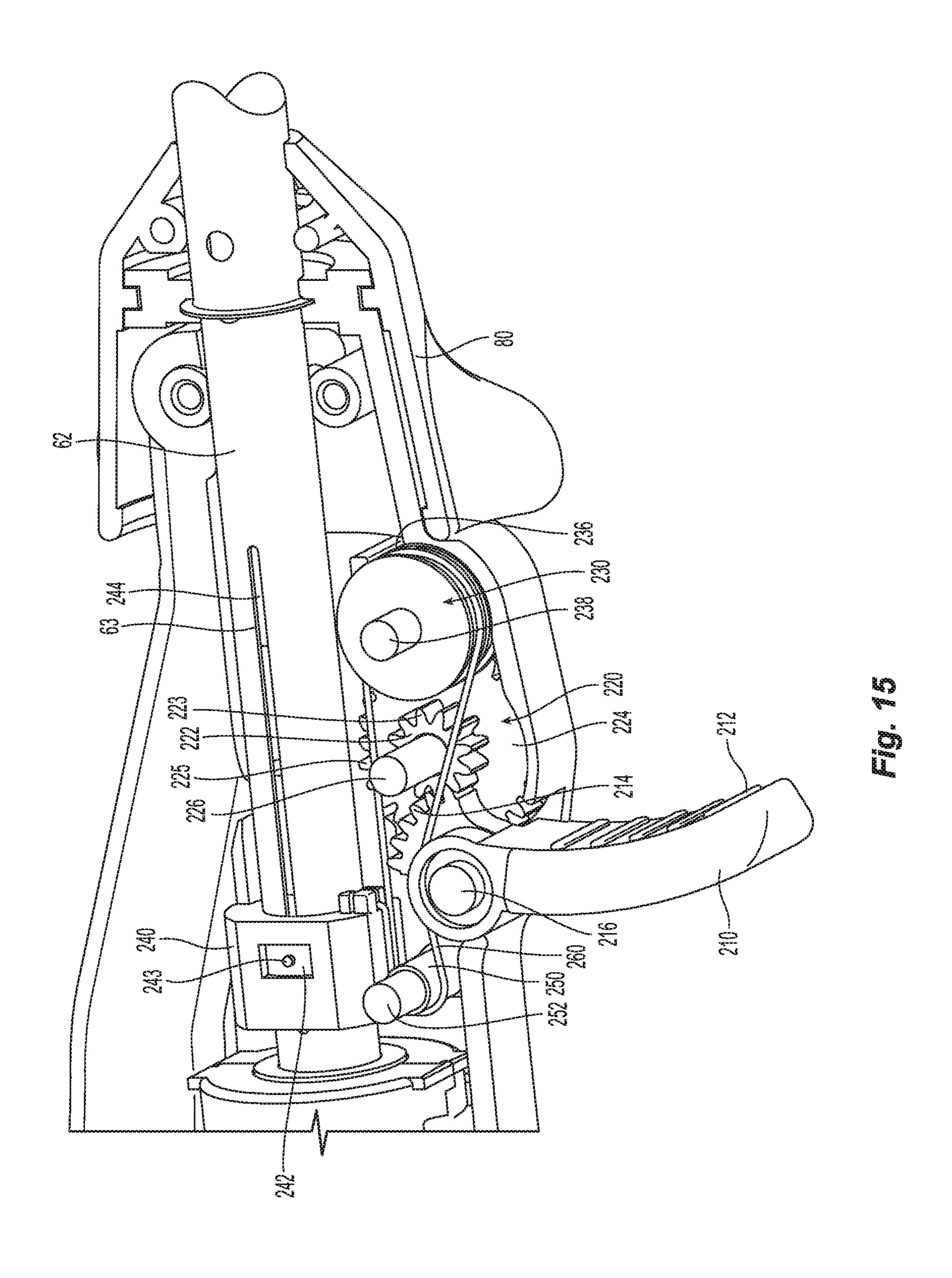


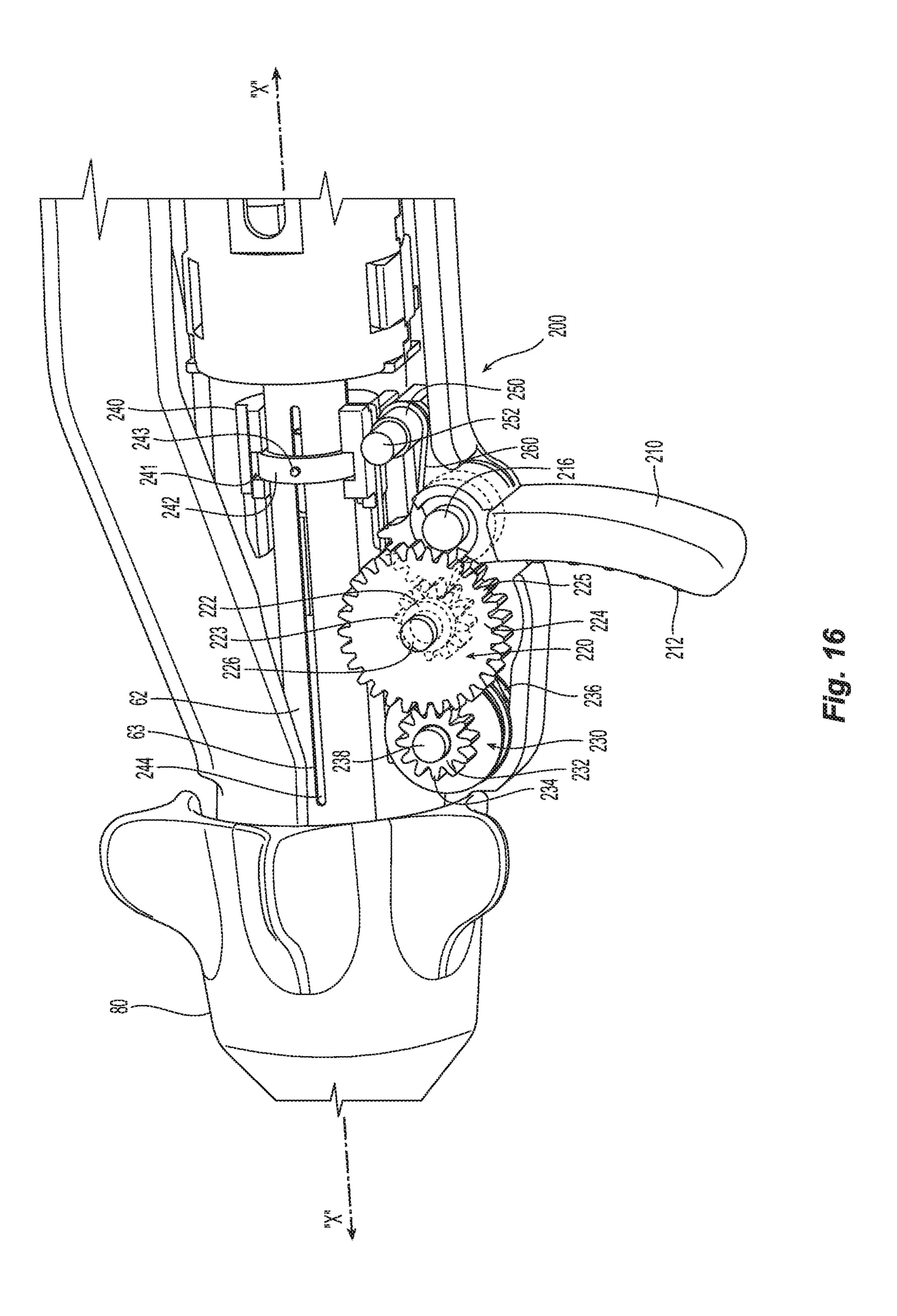


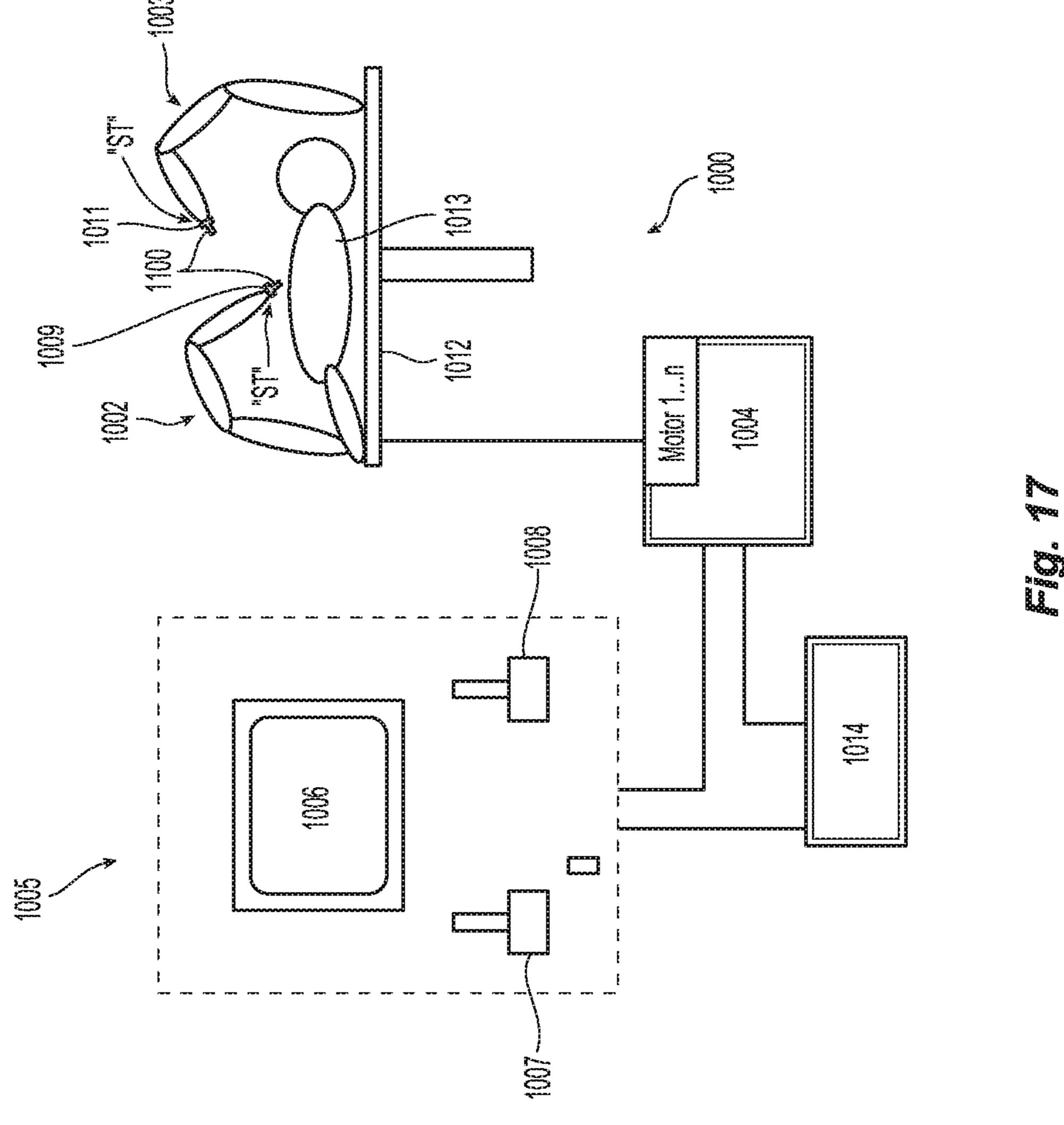












SURGICAL FORCEPS

CROSS REFERENCE TO RELATED APPLICATION

The present application claims the benefit of and priority to U.S. Provisional Application Ser. No. 62/376,434, filed on Aug. 18, 2016 the entire contents of which are incorporated herein by reference.

BACKGROUND

Technical Field

The present disclosure relates to surgical forceps and, ¹⁵ more particularly, to an endoscopic surgical forceps configured for treating and/or cutting tissue.

Background of Related Art

A surgical forceps is a pliers-like device which relies on mechanical action between its jaw members to grasp, clamp, and constrict tissue. Typically, at least one handle or lever is used to open and close the jaw members, and to provide compression force on tissue between the jaw members, to lock the jaw members in a closed position, and/or to apply energy to the jaw members to seal the tissue disposed therebetween.

Generally, such handles and levers used on surgical instruments are one of two types. One type is a simple ³⁰ pivoted handle that provides a near constant mechanical advantage throughout its stroke, and which is useful in many surgical situations. The second type of handle includes an additional link to provide a geometrically increasing mechanical advantage toward the end of its stroke to help ³⁵ provide the force necessary to compress tissue.

Both of these types of handles fix the mechanical advantage of the drive system such that the drive system cannot be optimized independently over the entire lever stroke. Often times, it may be desirable for a system to include fine 40 dissection capability (a relatively large amount of handle travel for a relatively small amount of jaw member movement) when the jaw members are in an initial, or open position, and to include a high mechanical advantage while applying compression force to tissue disposed between the 45 jaw members when the jaw members are in or near their approximated position (to help reduce surgeon fatigue, for instance). However, current handles are generally unable to achieve both of these desires in a single system.

SUMMARY

The present disclosure relates to a surgical instrument including a housing, an elongated shaft extending distally from the housing and defining a longitudinal axis, an end effector assembly, and a trigger assembly. The end effector assembly is disposed adjacent a distal end of the elongated shaft, and includes a first jaw member and a second jaw member. One or both of the jaw members is movable with respect to the other jaw member from a spaced-apart position to a position closer to the other jaw member for grasping tissue. The trigger assembly is disposed in mechanical cooperation with the housing and is configured to longitudinally translate a drive member. The trigger assembly is shown includes a trigger, a gear assembly, a spool, a slider, and a flexible drive member. The flexible drive of the harmonical cooperation with the gear assembly. The flexible drive

2

member is configured to engage the gear assembly, the spool, and the slider. Movement of the trigger with respect to the housing results in movement of the flexible drive member with respect to the housing and longitudinal movement of the slider with respect to the housing.

In aspects of the present disclosure, the surgical instrument further includes a drive assembly disposed at least partially within the housing. The drive assembly includes a drive bar extending at least partially through the elongated shaft such that longitudinal translation of the drive bar causes the jaw members to move between the spaced-apart position and the closer position for grasping tissue.

In other aspects, the drive bar is rotatable about the longitudinal axis with respect to the housing. In yet other aspects, the drive bar is rotatable about the longitudinal axis with respect to the slider.

In still other aspects, the trigger assembly further includes a ring. The ring is rotationally supported by the slider. In aspects of the present disclosure, the ring is rotationally fixed with respect to the drive bar. In other aspects, the ring is longitudinally translatable with respect to the drive bar.

In yet other aspects, the drive member is longitudinally translatable with respect to the drive bar. In still other aspects, the drive bar is rotatable with respect to the drive member.

In aspects of the present disclosure, the gear assembly includes a first gear and a second gear. The first gear is configured to engage the trigger, and the second gear is configured to engage the spool.

The present disclosure also relates to a trigger assembly for use with a surgical instrument. The trigger assembly includes a trigger, a gear assembly disposed in mechanical cooperation with the trigger, a spool, a slider, and a flexible drive member. The flexible drive member is configured to engage the gear assembly, the spool, and the slider. Actuation of the trigger results in movement of the flexible drive member with respect to the spool and longitudinal movement of the slider with respect to the spool.

In aspects of the present disclosure, the trigger assembly includes a ring rotationally supported by the slider. In other aspects, the ring is longitudinally translatable with respect to the spool.

In still other aspects, the gear assembly includes a first gear and a second gear. The first gear is configured to engage the trigger, and the second gear is configured to engage the spool. In yet other aspects, the first gear and the second gear are rotationally fixed with respect to each other.

In aspects of the present disclosure, the flexible drive member is in contact with the spool and the slider.

In other aspects, the spool includes a spool gear having a plurality of teeth configured to engage a portion of the gear assembly.

BRIEF DESCRIPTION OF THE DRAWINGS

Various aspects of the present disclosure are described herein with reference to the drawings wherein like reference numerals identify similar or identical elements:

FIG. 1 is a perspective view of a surgical forceps provided in accordance with the present disclosure;

FIG. 2 is a sectional view of a handle assembly of the surgical forceps of FIG. 1 where a first cam of a first handle is shown, and where a second cam of a second handle is omitted:

FIGS. 3-6 are perspective views of internal components of the handle assembly of FIGS. 1 and 2;

FIG. 6A is a perspective view of internal components of a handle assembly according to an embodiment of the present disclosure;

FIG. 7 is a sectional view of internal components of the handle assembly of FIGS. 1-6;

FIG. 8 is a sectional view of another embodiment of a surgical forceps provided in accordance with the present disclosure;

FIGS. 9-12 are perspective views of internal components of a handle assembly of the surgical forceps of FIG. 8;

FIG. 13 is a sectional view of a handle assembly of another embodiment of a surgical forceps provided in accordance with the present disclosure;

FIG. 14 is a sectional view of a trigger assembly of the surgical forceps of FIG. 13;

FIGS. 15 and 16 are perspective views of the trigger assembly of the surgical forceps of FIGS. 13-14; and

FIG. 17 is a schematic illustration of a surgical system in accordance with the present disclosure.

DETAILED DESCRIPTION

Embodiments of the presently disclosed surgical forceps are described in detail with reference to the drawings, in 25 which like reference numerals designate identical or corresponding elements in each of the several views. As used herein the term "distal" refers to that portion of the surgical forceps that is farther from the user, while the term "proximal" refers to that portion of the surgical forceps that is 30 closer to the user.

With initial reference to FIG. 1, an embodiment of a surgical forceps in accordance with the present disclosure is shown generally identified by reference character 10. connection with endoscopic surgical procedures, the present disclosure is equally applicable for surgical instruments used in open surgical procedures and in connection with any suitable surgical instrument. For the purposes herein, forceps 10 is generally described.

Forceps 10 is adapted for use in various surgical procedures and generally includes a housing 20, a handle assembly 30, a trigger assembly 70, a rotating assembly 80, and an end effector assembly 100. Jaw members 110 and 120 of end effector assembly 100 mutually cooperate to grasp, treat, 45 seal and/or cut tissue. Forceps 10 further includes a shaft 12 having a distal end 16 that mechanically engages end effector assembly 100, and a proximal end 14 that mechanically engages housing 20. Forceps 10 may be configured to connect to a source of energy, e.g., a generator (not shown), 50 tion. forceps 10 may be configured as a battery powered instrument, or forceps 10 may be manually powered (e.g., when providing electrosurgical energy is not desired).

As shown in FIGS. 1 and 2, for example, handle assembly 30 includes a first movable handle 30a and a second mov- 55 able 30b disposed on opposite sides of housing 20. Handles 30a and 30b are movable relative to one another to actuate end effector assembly 100, as will be described in greater detail below. Further, while two movable handles 30a and **30**b are shown and described herein, the present disclosure 60 also includes handle assembly 30 including a single movable handle, as shown in FIGS. 3-16, for example. Here, in addition to the single movable handle, a finger loop 34 is included on the opposite side of housing 20 as the single movable handle. Additionally, handle 30b may include the 65 same, mirror-image, or corresponding features as handle **30***a*.

Rotating assembly **80** is mechanically coupled to housing 20 and is rotatable in either direction, to rotate shaft 12 and, thus, end effector assembly 100 about a longitudinal axis "X" defined by shaft 12. Such a configuration allows end effector assembly 100 to be rotated in either direction with respect to housing 20.

Handle(s) 30a and/or 30b of handle assembly 30 ultimately connect to a drive assembly 60 disposed within housing 20 and that extends through shaft 12 which, together, cooperate to impart movement of jaw members 110 and 120 from an open position wherein jaw members 110 and 120 are disposed in spaced relation relative to one another, to a closed or approximated position wherein jaw members 110 and 120 cooperate to grasp tissue therebe-

Handles 30a and 30b of handle assembly 30 each include a finger loop or an aperture 33a and 33b, respectively, defined therein which enables a user to grasp and move handles 30a and 30b relative to one another and relative to 20 housing **20** between a spaced-apart position and an approximated position. In the embodiment where handle assembly 30 includes two handles 30a and 30b, each handle 30a and **30***b* is pivotably coupled to housing **20** at its respective distal end 31a, 31b via pivot pins 34a, 34b, respectively, and extends proximally to proximal ends 32a, 32b, respectively, thereof. As mentioned above, handles 30a, 30b are coupled to drive assembly 60 such that pivoting of handles 30a, 30b about pivot pins 34a, 34b, respectively, and relative to one another effects pivoting of jaw members 110, 120 between the open and closed positions, as discussed in further detail below. In the embodiment where handle assembly 30 includes a single movable handle 30a and a finger loop 34, handle 30a is pivotably coupled to housing at its distal end 31a via pivot pin 34b. Here, movement of handle 30a with Although surgical forceps 10 is shown configured for use in 35 respect to housing 20 effects pivoting of jaw members 110, 120 between the open and closed positions.

> With particular reference to FIG. 2, drive assembly 60 includes a drive bar 62 defining a proximal end 62a disposed within housing 20 and a distal end 62b that extends through 40 shaft 12, ultimately coupling to jaw members 110, 120. A mandrel **64** disposed within housing **20** is engaged with the proximal end 62a of drive bar 62. Mandrel 64 is slidably engaged with at least one track 22 (see FIG. 2) defined within housing 20 to guide longitudinal translation of mandrel 64 and, thus, drive bar 62, relative to housing 20. Other suitable guide/alignment mechanisms are also contemplated. A spring 69 is positioned within mandrel 64 and is configured to prevent over compression of tissue when jaw members 110, 120 are in the closed or approximated posi-

A follower 75 is rotatably supported by an axle 76, which extends through a bore of follower 75. Axle 76 is supported (e.g., rotatably supported) by proximal extensions 64a, 64b of mandrel **64**. A cam follower (e.g., a pin within a sleeve) 65 is also supported (e.g., rotatably supported) by proximal extensions 64a, 64b of mandrel 64.

While the following description discusses the use of two handles 30a, 30b, the use of a single handle 30a may also be utilized without departing from the scope of the present disclosure. In order to move jaw members 110, 120 from the open position to the closed position, handles 30a and/or 30b are squeezed, e.g., pivoted about pivot pins 34a, 34b, inwardly towards one another and housing 20. As handle(s) 30a, 30b are pivoted in this manner, proximal ends 32a, 32b of handles 30a, 30b are approximated relative to housing 20 and one another. The approximation of proximal ends 32a, 32b of handles 30a, 30b towards one another causes exten-

sions 140a, 140b of respective handles 30a, 30b to urge follower 75, mandrel 64 and drive bar 62 proximally, thus approximating jaw members 110, 120. Movement of handles 30a, 30b toward their open position causes extensions 140a, 140b to urge cam follower 65, mandrel 64 and 5 drive bar 62 distally, thus causing jaw members 110, 120 to move toward their open position, as further described below. The spring force of spring 69 may be configured such that jaw members 110, 120 impart a closure force between jaws within a range of about 3 kg/cm² to about 16 kg/cm², 10 although other closure forces are also contemplated.

Additionally, with reference to FIGS. 3-6, extension 140a includes a rib 150 thereon. The shape of rib 150 is arcuate when used with a pivoting handle 30a; rib 150 may be linear when used with a non-pivoting handle (not shown). Rib 150 is configured to be contacted by a roller 160.

As shown in FIGS. 4-6, roller 160 is supported by a support 170. Support 170 is fixed to housing 20 of surgical forceps 10 and includes a pin 172 extending through a leg 174 of support 170. Pin 172 rotationally supports roller 160. 20 Roller 160 is longitudinally fixed with respect to housing 20 and is configured to engage rib 150 of extension 140a.

As handle 30a, and thus extension 140a, is moved, roller 160 moves along rib 150. More particularly, as handle 30a is moved, roller 160 contacts and thus supports a distal wall 25 152 of rib 150. For example, when handle 30a is moved generally downward (as viewed in FIG. 3) to approximate the jaw members, for instance, roller 160 contacts distal wall 152 of rib 150. Thus, roller 160 provides support to rib 150, and thus handle 30a, during approximation of jaw members, 30 e.g., to restrict or minimize unintended bending or flexing motion in extension 140a, handle 30a, and other features within housing 20.

An alternate embodiment is shown in FIG. 6A, which includes a first roller 160a and a second roller 160b. Each of 35 first roller 160a and second roller 160b is supported by support 170. Support 170 is fixed to housing 20 of surgical forceps 10 and includes a first pin 172a and a second pin 172b extending through leg 174 of support 170. First pin 172a rotationally supports first roller 160a, and second pin 40 172b rotationally supports second roller 160b. First and second rollers 160a, 160b are longitudinally fixed with respect to housing 20 and are configured to engage rib 150 of extension 140a.

As handle 30a, and thus extension 140a, is moved, first 45 and second rollers 160a, 160b move along rib 150. More particularly, as handle 30a is moved, first roller 160a contacts and thus supports distal wall 152 of rib 150. For example, when handle 30a is moved generally downward (as viewed in FIG. 3) to approximate the jaw members, for 50 instance, first roller 160a contacts distal wall 152 of rib 150. Thus, first roller 160a provides support to rib 150, and thus handle 30a, during approximation of jaw members, e.g., to restrict or minimize unintended bending or flexing motion in extension 140a, handle 30a, and other features within housing 20. Additionally, when handle 30a is moved generally upward (as viewed in FIG. 3) to open the jaw members, for instance, second roller 160b contacts a proximal wall 152bof rib 150. Thus, second roller 160b provides support to rib 150, and thus handle 30a, during opening of jaw members, 60 e.g., to restrict or minimize unintended bending or flexing motion in extension 140a, handle 30a, and other features within housing **20**.

During use, a surgeon may desire fine (vs. gross) control of jaw members 110, 120 during some stages of use. For 65 example, the surgeon may wish to have greater control of the movement of the jaw members 110, 120 during dissection of

6

tissue, manipulation of tissue, and precise placement of jaw members 110, 120 about target tissue. For such fine control of jaw members 110, 120, a relative large amount of travel of handles 30a, 30b (or a single handle) would correspond to a relative small amount of travel of jaw members 110, 120. Some surgeons may also desire to have a high mechanical advantage during other stages of use. For example, a surgeon may wish to utilize a high mechanical advantage while applying compression force to tissue. To achieve such a high mechanical advantage, a relative small amount of travel of handles 30a, 30b would correspond to a relative large amount of travel of jaw members 110, 120. Typically, surgical instruments only allow for either fine control of jaw members 110, 120 or a high mechanical advantage. Examples of one surgical forceps configured to allow both fine control of jaw members and a high mechanical advantage at different stages of the actuation stroke of handles is described in U.S. Provisional Patent Application Ser. No. 62/247,279, filed on Oct. 28, 2015, the entire contents of which is incorporated by reference herein.

With particular reference to FIG. 7, to help ensure that contact is maintained between follower 75 and a proximal cam surface 142a, and between cam follower 65 and a distal cam surface 148a (e.g., to account for manufacturing tolerances, and/or to allow greater manufacturing tolerances, thus reducing costs), surgical forceps 10 may include an engagement spring 180 disposed between a proximal wall 64c of mandrel 64 and cam follower 65. Engagement spring 180 is configured to urge cam follower 65 proximally toward and into contact with distal cam surface 148a. Engagement spring 180 may be cone-like (e.g., frusto-conical) in shape, or a so-called Belleville washer.

With particular reference to FIGS. **8-12**, an additional An alternate embodiment is shown in FIG. **6A**, which includes a first roller **160***a* and a second roller **160***b*. Each of first roller **160***a* and second roller **160***b* is supported by support **170**. Support **170** is fixed to housing **20** of surgical with particular reference to FIGS. **8-12**, an additional embodiment of surgical forceps is shown and is indicated by reference character **2000**. Surgical forceps **2000** is similar to surgical forceps **10** discussed above and only the differences are discussed in detail herein.

Surgical forceps 2000 includes a movable handle 2030a and a finger loop 2030b. In lieu of finger loop 2030b, surgical forceps 2000 may include a second movable handle. Handle 2030a includes an extension 2032 having a groove or channel 2040 defined therein. A roller 2050 is movably positioned within channel 2040.

More particularly, channel 2040 extends within extension 2032 of handle 2030a and is defined by a proximal wall 2042 and a distal wall 2044 (FIG. 11). The shape of channel 2040 is arcuate when used with a pivoting handle 2030a; channel 2040 may be linear when used with a non-pivoting handle (not shown). Channel 2040 includes a width "wc" (FIG. 12) which may be uniform along its entire length or which may vary along at least a portion of its length.

Roller 2050 is supported by a support 2060. Support 2060 is fixed to housing 2002 of surgical forceps 2000 and includes a pin 2062 extending through a leg 2064 of support 2060. Pin 2062 rotationally supports roller 2050. Roller 2050 is longitudinally fixed with respect to housing 2002 and is configured to engage channel 2040 of extension 2032. Roller 2050 includes a width in the longitudinal direction. The width of roller 2050 is smaller than width "wc" of channel 2040, thus enabling roller 2050 to move within channel 2040.

As handle 2030a, and thus extension 2032, is moved, roller 2050 moves within channel 2040. More particularly, as handle 2030a is moved, roller 2050 contacts proximal wall 2042 and distal wall 2044 of channel 2040. For example, when handle 2030a is moved generally downward (as viewed in FIG. 8) to approximate the jaw members, for

instance, roller 2050 may contact distal wall 2044 of channel 2040; when handle 2030a is moved generally upward (as viewed in FIG. 8) to move the jaw members to the open position, for example, roller 2050 may contact proximal wall 2042 of channel 2040. Thus, channel 2040 provides support 5 to roller 2050 at all times during manipulation of the jaw members, e.g., to restrict or minimize unintended bending motion.

The difference between the width of roller 2050 and the width "wc" of channel **2040** determines the amount of travel 10 or "play" that handle 2030a can undergo while being actuated; a small difference between these distances results in a lower amount of "play."

Surgical forceps 10, 2000 may also include features to help maintain the handle(s) in the closed position, and may 15 include features for providing feedback to the user at certain stages of approximating or opening the jaw members. Such features are described in U.S. Provisional Patent Application Ser. No. 62/247,279, filed on Oct. 28, 2015, the entire contents of which have been incorporated by reference 20 hereinabove.

The present disclosure also includes methods of manipulating jaw members 110, 120 using fine and gross controls, as described above. For example, disclosed methods include moving handle 30a, 30b of surgical instrument 10 from a 25 non-actuated position a first distance to an intermediate position to cause first jaw member 110 to move a first amount, and moving handle 30a, 30b from the intermediate position a second distance to a fully actuated position to cause first jaw member 110 to move a second amount. Here, 30 the first distance is the same as the second distance, and the first amount is less than the second amount, thus resulting in an initial fine movement of jaw member 110, and a subsequent gross movement of jaw member 110.

second type of trigger assembly 200 are shown. Trigger assembly 200 of this embodiment includes a trigger 210, a gear assembly 220, a drive spool 230, a knife slider 240, a roller 250, and a flexible drive member 260. As discussed below, actuation of trigger assembly 200 is configured to 40 longitudinally translate a drive member (e.g., a knife drive shaft 244). Additionally, while trigger assembly 200 is shown used in connection with a particular surgical forceps 2000, trigger assembly 200 may also be used in connection with surgical forceps 10, or an additional type of surgical 45 device.

With particular reference to FIGS. 14 and 15, trigger 210 includes an actuation portion 212 configured for direct engagement by the user (e.g., physician), a plurality of trigger teeth 214, and is rotatable about a trigger pin 216. Gear assembly 220 (e.g., a cluster gear) includes a first gear 222 having a plurality of teeth 223, and a second gear 224 having a plurality of teeth 225. First gear 222 and second gear 224 are rotationally fixed with respect to each other, and are rotatable about a gear pin 226.

Drive spool 230 includes a spool gear 232 having a plurality of teeth 234 (see FIG. 16), and spool portion 236. Drive spool 230 is rotatable about a spool pin 238. A knife ring 242 is rotationally disposed within a portion of knife slider 240. Knife ring 242 is rotatable about the longitudinal 60 axis "X" with respect to knife slider 240. Roller 250 is rotatable about a roller pin 252. Flexible drive member 260 is in contact with spool portion 236 of drive spool 230, knife slider 240, and roller 250. Flexible drive member 260 can be made from any suitable material such as nylon, a para- 65 aramid synthetic fiber (e.g., Kevlar®), high-modulus polyethylene (HMPE), etc. for example. Flexible drive member

260 can also be made from plastic, e.g., having a rectangular cross-section (such as a zip-tie). In such embodiments, the pushing of various elements may be facilitated due to the strength of plastic. Additionally, assembly of surgical forceps 2000 may be facilitated using a plastic flexible drive member 260, for example, as fewer loops may be necessary to accomplish each desired action (e.g., proximal and distal translation of knife slider 240.

Details regarding the various interactions between the components of trigger assembly 200 are discussed herein with continued reference to FIGS. 13-16. Trigger teeth 214 of trigger 210 engage or mesh with teeth 223 of first gear 222 of gear assembly 220. Accordingly, movement of actuation portion 212 in the general direction of arrow "A" in FIGS. 13 and 14 causes rotation of trigger teeth 214 about trigger pin 216 in the general direction of arrow "B" in FIGS. 13 and 14, which causes rotation of first gear 222 about gear pin 226 in the general direction of arrow "C" in FIGS. 13 and **14**.

First gear 222 of gear assembly 220 is rotationally fixed with respect to second gear 224 of gear assembly 220. Teeth 225 of second gear 224 of gear assembly 220 engage or mesh with teeth 234 of spool gear 232 of drive spool 230. Accordingly, rotation of first gear 222 about gear pin 226 in the general direction of arrow "C" causes rotation of second gear 224 about gear pin 226 in the general direction of arrow "C," which causes rotation of spool gear **232** and drive spool 230 about spool pin 238 in the general direction of arrow "D" in FIGS. 13 and 14. Spool portion 236 of drive spool 230 is rotationally fixed with respect to spool gear 232, such that rotation of spool gear 232 causes a corresponding rotation of drive spool 230.

Flexible drive member 260 extends at least partially around spool portion 236 of drive spool 230, extends at least With particular reference to FIGS. 13-16, details of a 35 partially around roller 250, and is engaged with (e.g., wrapped around) a portion of knife slider 240. Flexible drive member 260 is longitudinally fixed with respect to knife slider 240. Accordingly, rotation of spool portion 236 of drive spool 230 in the general direction of arrow "D" causes translation of flexible drive member 260 in the general direction of arrow "E" in FIGS. 13 and 14, which causes roller 250 to rotate about roller pin 252 in the general direction of arrow "F" in FIGS. 13 and 14. Additionally, based on the way flexible drive member 260 engages a portion of knife slider 240 (as shown in FIG. 15), translation of flexible drive member 260 in the general direction of arrow "E" causes knife slider **240** to move in the general direction of arrow "G" (or distally) in FIGS. 13 and 14.

> Further, and with continued reference to FIG. 16, knife slider 240 includes a cutout 241 that rotationally supports knife ring 242, such that knife ring 242 is rotatable about the longitudinal axis "X" with respect to knife slider 240 and with respect to trigger 210, for example. Additionally, knife ring 242 is pinned to a knife drive shaft 244 and to drive bar 55 **62** by a ring pin **243**, such that rotation of rotating assembly 80 causes rotation of drive bar 62 and knife ring 242 about the longitudinal axis "X" with respect to knife slider 240. Moreover, ring pin 243 extends through a longitudinal slot 63 of drive bar 62. Thus, longitudinal translation of knife slider 240 causes a corresponding longitudinal translation of knife ring 242 and knife drive shaft 244.

Accordingly, actuation of trigger 210 in a first direction (e.g., in the general direction of arrow "A") causes rotation of gear assembly 220, rotation of drive spool 230, movement of flexible drive member 260 around spool portion 236 of drive spool 230 and around roller 250, which causes distal translation or advancement of knife slider 240, knife ring

242 and knife drive shaft 244 to cut tissue, for example. Additionally, movement of trigger 210 in a second direction (e.g., in the general opposite direction of arrow "A") causes proximal translation or retraction of knife drive shaft 244.

Additionally, while the illustrated embodiments depict 5 one type of surgical instrument (i.e., surgical forceps), the present disclosure includes the use of various features described herein in connection with other types of surgical devices including at least one pivotable handle or lever. For instance, various handle assemblies for actuating handle(s) 10 and corresponding drive assemblies are contemplated for translating drive bar **62** and are discussed in commonly-owned U.S. Pat. No. 7,857,812, the entire contents of which are incorporated by reference herein.

Additionally, further details of a surgical forceps having a similar handle assembly to the disclosed handle assembly 30 are disclosed in U.S. Pat. No. 8,430,876, the entire contents of which being incorporated by reference herein. Further details of an electrosurgical instrument are disclosed in U.S. Pat. Nos. 7,101,371 and 7,083,618, the entire contents of 20 which being incorporated by reference herein.

The various embodiments disclosed herein may also be configured to work with robotic surgical systems and what is commonly referred to as "Telesurgery." Such systems employ various robotic elements to assist the surgeon and 25 allow remote operation (or partial remote operation) of surgical instrumentation. Various robotic arms, gears, cams, pulleys, electric and mechanical motors, etc. may be employed for this purpose and may be designed with a robotic surgical system to assist the surgeon during the 30 course of an operation or treatment. Such robotic systems may include remotely steerable systems, automatically flexible surgical systems, remotely articulating surgical systems, wireless surgical systems, modular or selectively configurable remotely operated surgical systems, etc.

The robotic surgical systems may be employed with one or more consoles that are next to the operating theater or located in a remote location. In this instance, one team of surgeons or nurses may prepare the patient for surgery and 40 configure the robotic surgical system with one or more of the surgical instruments disclosed herein while another surgeon (or group of surgeons) remotely controls the instrument(s) via the robotic surgical system. As can be appreciated, a highly skilled surgeon may perform multiple operations in 45 multiple locations without leaving his/her remote console which can be both economically advantageous and a benefit to the patient or a series of patients.

The robotic arms of the surgical system are typically coupled to a pair of master handles by a controller. The 50 handles can be moved by the surgeon to produce a corresponding movement of the working ends of any type of surgical instrument (e.g., end effectors, graspers, knifes, scissors, etc.) which may complement the use of one or more of the embodiments described herein. The movement of the 55 master handles may be scaled so that the working ends have a corresponding movement that is different, smaller or larger, than the movement performed by the operating hands of the surgeon. The scale factor or gearing ratio may be adjustable so that the operator can control the resolution of 60 the working ends of the surgical instrument(s).

The master handles may include various sensors to provide feedback to the surgeon relating to various tissue parameters or conditions, e.g., tissue resistance due to manipulation, cutting or otherwise treating, pressure by the 65 instrument onto the tissue, tissue temperature, tissue impedance, etc. As can be appreciated, such sensors provide the

10

surgeon with enhanced tactile feedback simulating actual operating conditions. The master handles may also include a variety of different actuators for delicate tissue manipulation or treatment further enhancing the surgeon's ability to mimic actual operating conditions.

With particular reference to FIG. 17, a medical work station is shown generally as work station 1000 and generally may include a plurality of robot arms 1002, 1003; a control device 1004; and an operating console 1005 coupled with control device 1004. Operating console 1005 may include a display device 1006, which may be set up in particular to display three-dimensional images; and manual input devices 1007, 1008, by means of which a person (not shown), for example a surgeon, may be able to telemanipulate robot arms 1002, 1003 in a first operating mode.

Each of the robot arms 1002, 1003 may include a plurality of members, which are connected through joints, and an attaching device 1009, 1011, to which may be attached, for example, a surgical tool "ST" supporting an end effector 1100, in accordance with any one of several embodiments disclosed herein, as will be described in greater detail below.

Robot arms 1002, 1003 may be driven by electric drives (not shown) that are connected to control device 1004. Control device 1004 (e.g., a computer) may be set up to activate the drives, in particular by means of a computer program, in such a way that robot arms 1002, 1003, their attaching devices 1009, 1011 and thus surgical instrument 10 (including end effector 300) execute a desired movement according to a movement defined by means of manual input devices 1007, 1008. Control device 1004 may also be set up in such a way that it regulates the movement of robot arms 1002, 1003 and/or of the drives.

Medical work station 1000 may be configured for use on a patient 1013 lying on a patient table 1012 to be treated in a minimally invasive manner by means of end effector 1100. Medical work station 1000 may also include more than two robot arms 1002, 1003, the additional robot arms likewise being connected to control device 1004 and being telemanipulatable by means of operating console 1005. A medical instrument or surgical tool (including an end effector 1100) may also be attached to the additional robot arm. Medical work station 1000 may include a database 1014, in particular coupled to with control device 1004, in which are stored, for example, pre-operative data from patient/living being 1013 and/or anatomical atlases.

From the foregoing and with reference to the various figure drawings, those skilled in the art will appreciate that certain modifications can also be made to the present disclosure without departing from the scope of the same. While several embodiments of the disclosure have been shown in the drawings, it is not intended that the disclosure be limited thereto, as it is intended that the disclosure be as broad in scope as the art will allow and that the specification be read likewise. Therefore, the above description should not be construed as limiting, but merely as exemplifications of particular embodiments. Those skilled in the art will envision other modifications within the scope and spirit of the claims appended hereto.

What is claimed is:

- 1. A surgical instrument, comprising: a housing;
- an elongated shaft extending distally from the housing and defining a longitudinal axis;
- an end effector assembly disposed adjacent a distal end of the elongated shaft, the end effector assembly including a first jaw member and a second jaw member, at least one of the jaw members movable with respect to the

- other jaw member from a spaced-apart position to a position closer to the other jaw member for grasping tissue; and
- a trigger assembly disposed in mechanical cooperation with the housing and configured to longitudinally translate a drive member, the trigger assembly including a trigger, a gear assembly, a spool, a slider, and a flexible drive member, the trigger disposed in mechanical cooperation with the gear assembly, the flexible drive member configured to engage the gear assembly, the spool, and the slider, the flexible drive member configured as a continuous loop, wherein movement of the trigger with respect to the housing results in movement of the flexible drive member with respect to the housing and longitudinal movement of the slider with respect to the housing.
- 2. The surgical instrument according to claim 1, further comprising a drive assembly disposed at least partially within the housing, the drive assembly including a drive bar extending at least partially through the elongated shaft such 20 that longitudinal translation of the drive bar causes the jaw members to move between the spaced-apart position and the closer position for grasping tissue.
- 3. The surgical instrument according to claim 2, wherein the drive bar is rotatable about the longitudinal axis with 25 respect to the housing.
- 4. The surgical instrument according to claim 2, wherein the drive bar is rotatable about the longitudinal axis with respect to the slider.
- 5. The surgical instrument according to claim 2, wherein 30 the trigger assembly further comprises a ring rotationally supported by the slider.
- 6. The surgical instrument according to claim 5, wherein the ring is rotationally fixed with respect to the drive bar.
- 7. The surgical instrument according to claim **6**, wherein 35 the ring is longitudinally translatable with respect to the drive bar.
- 8. The surgical instrument according to claim 5, wherein the ring is rotatable relative to the housing.
- 9. The surgical instrument according to claim 5, wherein 40 the slider is rotationally fixed relative to the housing.
- 10. The surgical instrument according to claim 2, wherein the drive member is longitudinally translatable with respect to the drive bar.

12

- 11. The surgical instrument according to claim 10, wherein the drive bar is rotatable with respect to the drive member.
- 12. The surgical instrument according to claim 1, wherein the gear assembly includes a first gear and a second gear, the first gear configured to engage the trigger, and the second gear configured to engage the spool.
- 13. A trigger assembly for use with a surgical instrument, the trigger assembly comprising:
 - a trigger;
 - a gear assembly disposed in mechanical cooperation with the trigger;
 - a spool;
 - a slider; and
 - a flexible drive member, the flexible drive member configured to engage the gear assembly, the spool, and the slider, wherein actuation of the trigger results in movement of the flexible drive member with respect to the spool and longitudinal movement of the slider with respect to the spool, wherein an amount of contact between the flexible drive member and the spool remains constant during actuation of the trigger.
- 14. The trigger assembly according to claim 13, further comprising a ring rotationally supported by the slider.
- 15. The trigger assembly according to claim 14, wherein the ring is longitudinally translatable with respect to the spool.
- 16. The trigger assembly according to claim 13, wherein the gear assembly includes a first gear and a second gear, the first gear configured to engage the trigger, and the second gear configured to engage the spool.
- 17. The trigger assembly according to claim 16, wherein the first gear and the second gear are rotationally fixed with respect to each other.
- 18. The trigger assembly according to claim 13, wherein the flexible drive member is in contact with the spool and the slider.
- 19. The trigger assembly according to claim 13, wherein the spool includes a spool gear having a plurality of teeth configured to engage a portion of the gear assembly.

* * * *