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(54) **SURGICAL FORCEPS**

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(56) **References Cited**

U.S. PATENT DOCUMENTS

D249,549 S 9/1978 Pike
D263,020 S 2/1982 Rau, III
(Continued)

FOREIGN PATENT DOCUMENTS

CN 201299462 Y 9/2009
DE 2415263 A1 10/1975
(Continued)

OTHER PUBLICATIONS

Heniford et al. "Initial Research and Clinical Results with an Electrothermal Bipolar Vessel Sealer" Oct. 1999.
(Continued)

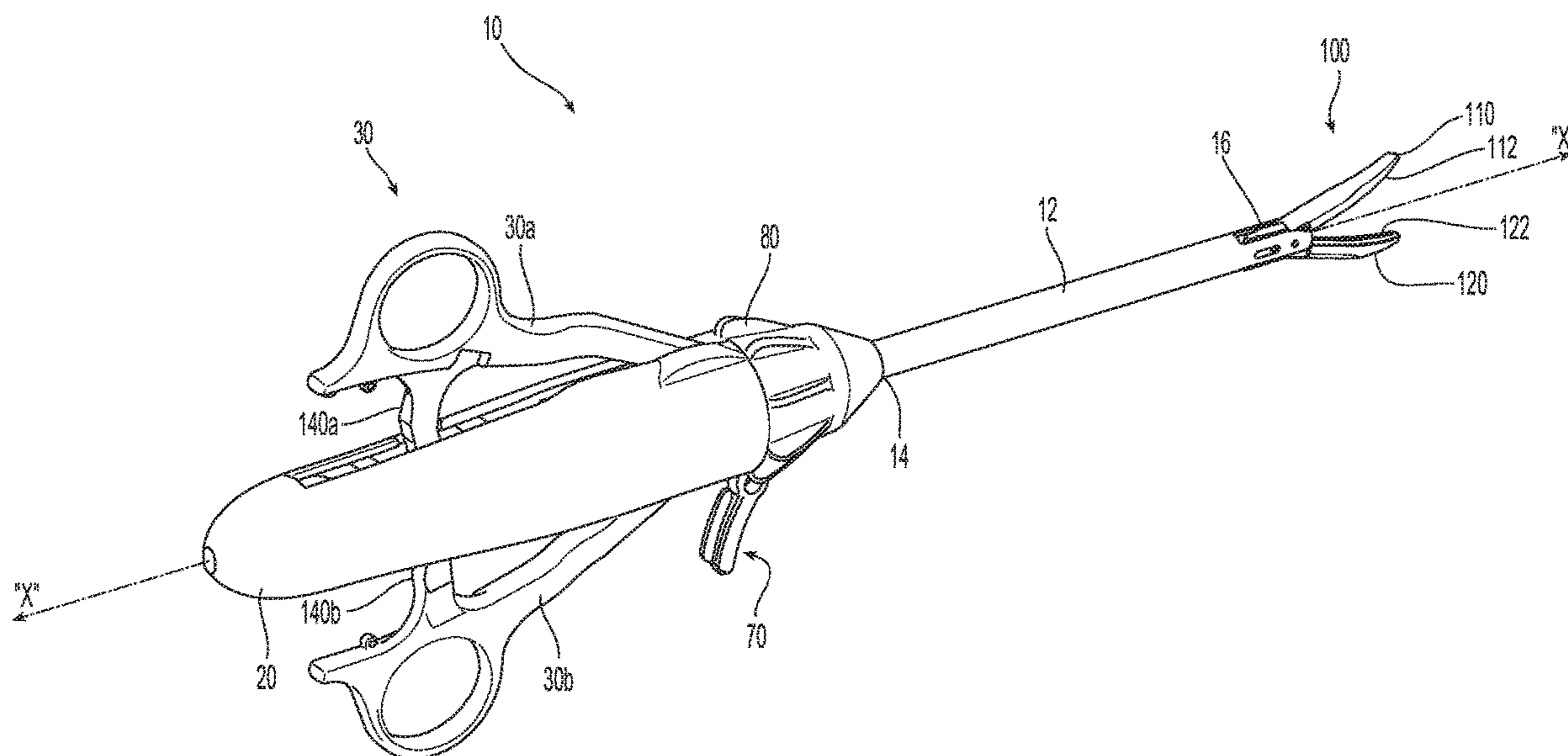
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(57) **ABSTRACT**

A surgical instrument includes a housing, an elongated shaft extending distally from the housing, an end effector assembly, and a trigger assembly. The trigger assembly is disposed in mechanical cooperation with the housing and is configured to longitudinally translate a drive member. The trigger assembly includes a trigger, a gear assembly, a spool, a slider, and a flexible drive member. The trigger is disposed in mechanical cooperation with the gear assembly. The flexible drive member is configured to engage the gear assembly, the spool, and the slider. Movement of the trigger with respect to the housing results in movement of the flexible drive member with respect to the housing and longitudinal movement of the slider with respect to the housing.

19 Claims, 18 Drawing Sheets



(51)	Int. Cl.		D617,901 S	6/2010	Unger et al.	
	<i>A61B 17/29</i>	(2006.01)	D617,902 S	6/2010	Twomey et al.	
	<i>A61B 17/32</i>	(2006.01)	D617,903 S	6/2010	Unger et al.	
	<i>A61B 17/295</i>	(2006.01)	D618,798 S	6/2010	Olson et al.	
	<i>A61B 18/14</i>	(2006.01)	D621,503 S	8/2010	Otten et al.	
	<i>A61B 17/3201</i>	(2006.01)	D627,462 S	11/2010	Kingsley	
	<i>A61B 34/30</i>	(2016.01)	D628,289 S	11/2010	Romero	
	<i>A61B 90/00</i>	(2016.01)	D628,290 S	11/2010	Romero	
(52)	U.S. Cl.		D630,324 S	1/2011	Reschke	
	CPC .. <i>A61B 17/320016</i>	(2013.01); <i>A61B 18/1445</i>	D649,249 S	11/2011	Guerra	
		(2013.01); <i>A61B 17/3201</i>	D649,643 S	11/2011	Allen, IV et al.	
		(2013.01); <i>A61B 17/3201</i>	D661,394 S	6/2012	Romero et al.	
		(2016.02); <i>A61B 90/03</i>	D670,808 S	11/2012	Moua et al.	
		(2016.02); <i>A61B 2017/00353</i>	D680,220 S	4/2013	Rachlin	
		(2013.01); <i>A61B 2017/2913</i>	9,084,608 B2	7/2015	Larson et al.	
		(2013.01); <i>A61B 2017/2915</i>	9,211,657 B2	12/2015	Ackley et al.	
		(2013.01); <i>A61B 2017/2915</i>	9,566,065 B2*	2/2017	Knodel	A61B 17/068
		(2013.01); <i>A61B 2018/1452</i>	2005/0209596 A1	9/2005	Daniels et al.	
		(2013.01)	2007/0175964 A1*	8/2007	Shelton, IV	A61B 17/072 227/180.1
(58)	Field of Classification Search		2010/0004677 A1	1/2010	Brostoff et al.	
	CPC .. <i>A61B 2017/00353</i> ; <i>A61B 2017/2923</i> ; <i>A61B</i>		2011/0276049 A1*	11/2011	Gerhardt	A61B 18/1402 606/45
			2012/0316601 A1	12/2012	Twomey	
			2014/0221995 A1	8/2014	Guerra et al.	
			2014/0221999 A1	8/2014	Cunningham et al.	
(56)	References Cited		2014/0228842 A1	8/2014	Dycus et al.	
	U.S. PATENT DOCUMENTS		2014/0230243 A1	8/2014	Roy et al.	
	D295,893 S	5/1988 Sharkany et al.	2014/0236149 A1	8/2014	Kharin et al.	
	D295,894 S	5/1988 Sharkany et al.	2014/0243811 A1	8/2014	Reschke et al.	
	D298,353 S	11/1988 Manno	2014/0243824 A1	8/2014	Gilbert	
	D299,413 S	1/1989 DeCarolis	2014/0249528 A1	9/2014	Hixson et al.	
	D343,453 S	1/1994 Noda	2014/0250686 A1	9/2014	Hempstead et al.	
	D348,930 S	7/1994 Olson	2014/0257274 A1	9/2014	McCullough, Jr. et al.	
	D349,341 S	8/1994 Lichtman et al.	2014/0257283 A1	9/2014	Johnson et al.	
	D354,564 S	1/1995 Medema	2014/0257284 A1	9/2014	Artale	
	D358,887 S	5/1995 Feinberg	2014/0257285 A1	9/2014	Moua	
	5,582,615 A *	12/1996 Foshee	2014/0276803 A1	9/2014	Hart	
		A61B 17/2909	2014/0284313 A1	9/2014	Allen, IV et al.	
		606/139	2014/0288549 A1	9/2014	McKenna et al.	
	D384,413 S	9/1997 Zlock et al.	2014/0288553 A1	9/2014	Johnson et al.	
	H1745 H	8/1998 Paraschac	2014/0330308 A1	11/2014	Hart et al.	
	D402,028 S	12/1998 Grimm et al.	2014/0332578 A1*	11/2014	Fernandez	A61B 17/068 227/175.1
	D408,018 S	4/1999 McNaughton	2014/0336635 A1	11/2014	Hart et al.	
	D416,089 S	11/1999 Barton et al.	2014/0339286 A1*	11/2014	Motooka	A61B 17/07207 227/175.2
	D424,694 S	5/2000 Tetzlaff et al.	2014/0353188 A1	12/2014	Reschke et al.	
	D425,201 S	5/2000 Tetzlaff et al.	2015/0018816 A1	1/2015	Latimer	
	H1904 H	10/2000 Yates et al.	2015/0025528 A1	1/2015	Arts	
	D449,886 S	10/2001 Tetzlaff et al.	2015/0032106 A1	1/2015	Rachlin	
	D453,923 S	2/2002 Olson	2015/0051598 A1	2/2015	Orszulak et al.	
	D454,951 S	3/2002 Bon	2015/0051640 A1	2/2015	Twomey et al.	
	D457,958 S	5/2002 Dycus et al.	2015/0066026 A1	3/2015	Hart et al.	
	D457,959 S	5/2002 Tetzlaff et al.	2015/0080880 A1	3/2015	Sartor et al.	
	H2037 H	7/2002 Yates et al.	2015/0080889 A1	3/2015	Cunningham et al.	
	D465,281 S	11/2002 Lang	2015/0082928 A1	3/2015	Kappus et al.	
	D466,209 S	11/2002 Bon	2015/0088122 A1	3/2015	Jensen	
	D493,888 S	8/2004 Reschke	2015/0088126 A1	3/2015	Duffin et al.	
	D496,997 S	10/2004 Dycus et al.	2015/0088128 A1	3/2015	Couture	
	D499,181 S	11/2004 Dycus et al.	2015/0094714 A1	4/2015	Lee et al.	
	D502,994 S	3/2005 Blake, III	2015/0209059 A1*	7/2015	Trees	A61B 18/1445 606/170
	D509,297 S	9/2005 Wells	2016/0135869 A1*	5/2016	Jadhav	F16H 19/06 606/52
	D525,361 S	7/2006 Hushka	2017/0143361 A1*	5/2017	Boudreaux	A61B 17/29
	D531,311 S	10/2006 Guerra et al.	2017/0143362 A1*	5/2017	Cagle	A61B 18/1445
	D533,274 S	12/2006 Visconti et al.				
	D533,942 S	12/2006 Kerr et al.				
	D535,027 S	1/2007 James et al.				
	D538,932 S	3/2007 Malik				
	D541,418 S	4/2007 Schechter et al.				
	D541,611 S	5/2007 Aglassinger				
	D541,938 S	5/2007 Kerr et al.				
	D545,432 S	6/2007 Watanabe				
	D547,154 S	7/2007 Lee				
	D564,662 S	3/2008 Moses et al.				
	D567,943 S	4/2008 Moses et al.				
	D575,395 S	8/2008 Hushka				
	D575,401 S	8/2008 Hixson et al.				
	D582,038 S	12/2008 Swoyer et al.				
	D617,900 S	6/2010 Kingsley et al.				

FOREIGN PATENT DOCUMENTS

DE	02514501	A1	10/1976
DE	2627679	A1	1/1977
DE	03423356	C2	6/1986
DE	03612646	A1	4/1987
DE	3627221	A1	2/1988
DE	8712328	U1	2/1988
DE	4211417	A1	10/1993
DE	04303882	C2	2/1995

(56)

References Cited

FOREIGN PATENT DOCUMENTS

DE	04403252	A1	8/1995
DE	19515914	C1	7/1996
DE	19506363	A1	8/1996
DE	29616210	U1	11/1996
DE	19608716	C1	4/1997
DE	19751106	A1	5/1998
DE	19738457	A1	3/1999
DE	19751108	A1	5/1999
DE	19946527	C1	7/2001
DE	10031773	A1	11/2001
DE	10045375	A1	4/2002
DE	20121161	U1	4/2002
DE	102004026179	A1	12/2005
DE	202007009165	U1	8/2007
DE	202007009318	U1	8/2007
DE	202007009317	U1	10/2007
DE	202007016233	U1	1/2008
DE	102008018406	B3	7/2009
EP	0589453	A2	3/1994
EP	1159926	A2	12/2001
EP	1281878	A1	2/2003
EP	2777586	A1	9/2014
EP	2890309	A1	7/2015
JP	61-501068		9/1984
JP	11-47150	A	6/1989
JP	6-502328		3/1992
JP	5-5106		1/1993
JP	05-40112		2/1993
JP	0006030945	A	2/1994
JP	6-121797	A	5/1994
JP	6-285078	A	10/1994
JP	6-511401		12/1994
JP	06343644	A	12/1994
JP	07265328	A	10/1995
JP	8-56955		3/1996
JP	08252263	A	10/1996
JP	8-289895	A	11/1996
JP	8-317934	A	12/1996
JP	8-317936	A	12/1996
JP	910223		1/1997
JP	09000538	A	1/1997
JP	9-122138	A	5/1997
JP	1024051		1/1998
JP	0010000195	A	1/1998
JP	10-155798	A	6/1998
JP	11-47149		2/1999
JP	11-070124	A	3/1999
JP	11-169381	A	6/1999
JP	11-192238	A	7/1999
JP	11244298	A	9/1999
JP	2000-102545	A	4/2000
JP	2000-135222	A	5/2000
JP	2000342599	A	12/2000
JP	2000350732	A	12/2000
JP	2001008944	A	1/2001
JP	2001-029355	A	2/2001
JP	2001029356	A	2/2001
JP	2001128990	A	5/2001
JP	2001-190564	A	7/2001
JP	2001-003400		11/2001
JP	2002-136525	A	5/2002
JP	2002-528166	A	9/2002
JP	2003-116871	A	4/2003
JP	2003-175052	A	6/2003
JP	2003245285	A	9/2003
JP	2004-517668	A	6/2004
JP	2004-528869	A	9/2004
JP	2005-152663	A	6/2005
JP	2005-253789	A	9/2005
JP	2005312807	A	11/2005
JP	2006-015078	A	1/2006
JP	2006-501939	A	1/2006
JP	2006-095316	A	4/2006
JP	2008-054926	A	3/2008
JP	2011125195	A	6/2011

SU	401367	A1	10/1973
WO	0036986	A1	6/2000
WO	0059392	A1	10/2000
WO	0115614	A1	3/2001
WO	0154604	A1	8/2001
WO	02/45589	A2	6/2002
WO	06/021269	A1	3/2006
WO	05110264	A3	4/2006
WO	08/040483	A1	4/2008
WO	2011/018154	A1	2/2011

OTHER PUBLICATIONS

Extended European Search Report for EP 16196110 dated Dec. 23, 2016.

Michael Choti, "Abdominoperineal Resection with the LigaSure Vessel Sealing System and LigaSure Atlas 20 cm Open Instrument"; Innovations That Work, Jun. 2003.

Chung et al., "Clinical Experience of Sutureless Closed Hemorrhoidectomy with LigaSure" Diseases of the Colon & Rectum vol. 46, No. 1 Jan. 2003.

Tinkler L.F., "Combined Diathermy and Suction Forceps", Feb. 6, 1967 (Feb. 6, 1967), British Medical Journal Feb. 6, 1976, vol. 1, nr. 5431 p. 361, ISSN: 0007-1447.

Carbonell et al., "Comparison of the Gyros PlasmaKinetic Sealer and the Valleylab LigaSure Device in the Hemostasis of Small, Medium, and Large-Sized Arteries" Carolinas Laparoscopic and Advanced Surgery Program, Carolinas Medical Center, Charlotte, NC; Date: Aug. 2003.

Peterson et al. "Comparison of Healing Process Following Ligation with Sutures and Bipolar Vessel Sealing" Surgical Technology International (2001).

"Electrosurgery: A Historical Overview" Innovations in Electrosurgery; Sales/Product Literature; Dec. 31, 2000. (6 pages).

Johnson et al. "Evaluation of a Bipolar Electrothermal Vessel Sealing Device in Hemorrhoidectomy" Sales/Product Literature; Jan. 2004. (1 page).

E. David Crawford "Evaluation of a New Vessel Sealing Device in Urologic Cancer Surgery" Sales/Product Literature 2000.

Johnson et al. "Evaluation of the LigaSure Vessel Sealing System in Hemorrhoidectomy" American College of Surgeons (ACS) Clinical Congress Poster (2000).

Muller et al., "Extended Left Hemicolectomy Using the LigaSure Vessel Sealing System" Innovations That Work, Sep. 1999.

Kennedy et al. "High-burst-strength, feedback-controlled bipolar vessel sealing" Surgical Endoscopy (1998) 12: 876-878.

Burdette et al. "In Vivo Probe Measurement Technique for Determining Dielectric Properties at VHF Through Microwave Frequencies", IEEE Transactions on Microwave Theory and Techniques, vol. MTT-28, No. 4, Apr. 1980 pp. 414-427.

Carus et al., "Initial Experience With the LigaSure Vessel Sealing System in Abdominal Surgery" Innovations That Work, Jun. 2002.

Heniford et al. "Initial Results with an Electrothermal Bipolar Vessel Sealer" Surgical Endoscopy (2000) 15:799-801. (4 pages).

Herman et al., "Laparoscopic Intestinal Resection With the LigaSure Vessel Sealing System: A Case Report"; Innovations That Work, Feb. 2002.

Koyle et al., "Laparoscopic Palomo Varicocele Ligation in Children and Adolescents" Pediatric Endosurgery & Innovative Techniques, vol. 6, No. 1, 2002.

W. Scott Helton, "LigaSure Vessel Sealing System: Revolutionary Hemostasis Product for General Surgery"; Sales/Product Literature 1999.

LigaSure Vessel Sealing System, the Seal of Confidence in General, Gynecologic, Urologic, and Laparoscopic Surgery; Sales/Product Literature; Apr. 2002.

Joseph Ortenberg "LigaSure System Used in Laparoscopic 1st and 2nd Stage Orchiopexy" Innovations That Work, Nov. 2002.

Sigel et al. "The Mechanism of Blood Vessel Closure by High Frequency Electrocoagulation" Surgery Gynecology & Obstetrics, Oct. 1965 pp. 823-831.

(56)

References Cited

OTHER PUBLICATIONS

Sampayan et al, "Multilayer Ultra-High Gradient Insulator Technology" Discharges and Electrical Insulation in Vacuum, 1998. Netherlands Aug. 17-21, 1998; vol. 2, pp. 740-743.

Paul G. Horgan, "A Novel Technique for Parenchymal Division During Hepatectomy" The American Journal of Surgery, vol. 181, No. 3, Apr. 2001 pp. 236-237.

Benaron et al., "Optical Time-Of-Flight and Absorbance Imaging of Biologic Media", Science, American Association for the Advancement of Science, Washington, DC, vol. 259, Mar. 5, 1993, pp. 1463-1466.

Olsson et al. "Radical Cystectomy in Females" Current Surgical Techniques in Urology, vol. 14, Issue 3, 2001.

Palazzo et al. "Randomized clinical trial of Ligasure versus open haemorrhoidectomy" British Journal of Surgery 2002, 89, 154-157.

Levy et al. "Randomized Trial of Suture Versus Electrosurgical Bipolar Vessel Sealing in Vaginal Hysterectomy" Obstetrics & Gynecology, vol. 102, No. 1, Jul. 2003.

"Reducing Needlestick Injuries in the Operating Room" Sales/Product Literature 2001. (1 page).

Bergdahl et al. "Studies on Coagulation and the Development of an Automatic Computerized Bipolar Coagulator" J. Neurosurg, vol. 75, Jul. 1991, pp. 148-151.

Strasberg et al. "A Phase I Study of the LigaSure Vessel Sealing System in Hepatic Surgery" Section of HPB Surger, Washington University School of Medicine, St. Louis MO, Presented at AHPBA, Feb. 2001.

Sayfan et al. "Sutureless Closed Hemorrhoidectomy: A New Technique" Annals of Surgery vol. 234 No. 1 Jul. 2001; pp. 21-24.

Levy et al., "Update on Hysterectomy—New Technologies and Techniques" OBG Management, Feb. 2003. (15 pages).

Dulemba et al. "Use of a Bipolar Electrothermal Vessel Sealer in Laparoscopically Assisted Vaginal Hysterectomy" Sales/Product Literature; Jan. 2004.

Strasberg et al., "Use of a Bipolar Vessel-Sealing Device for Parenchymal Transection During Liver Surgery" Journal of Gastrointestinal Surgery, vol. 6, No. 4, Jul./Aug. 2002 pp. 569-574.

Sengupta et al., "Use of a Computer-Controlled Bipolar Diathermy System in Radical Prostatectomies and Other Open Urological

Surgery" ANZ Journal of Surgery (2001) 71.9 pp. 538-540.

Rothenberg et al. "Use of the LigaSure Vessel Sealing System in Minimally Invasive Surgery in Children" Int'l Pediatric Endosurgery Group (IPEG) 2000.

Crawford et al. "Use of the LigaSure Vessel Sealing System in Urologic Cancer Surgery" Grand Rounds in Urology 1999 vol. 1 Issue 4 pp. 10-17.

Craig Johnson, "Use of the LigaSure Vessel Sealing System in Bloodless Hemorrhoidectomy" Innovations That Work, Mar. 2000.

Levy et al. "Use of a New Energy-based Vessel Ligation Device During Vaginal Hysterectomy" Int'l Federation of Gynecology and Obstetrics (FIGO) World Congress 1999.

Barbara Levy, "Use of a New Vessel Ligation Device During Vaginal Hysterectomy" FIGO 2000, Washington, D.C.. (1 page).

E. David Crawford "Use of a Novel Vessel Sealing Technology in Management of the Dorsal Venous Complex" Sales/ Product Literature 2000.

Jarrett et al., "Use of the LigaSure Vessel Sealing System for Peri-Hilar Vessels in Laparoscopic Nephrectomy" Sales/Product Literature 2000.

Crouch et al. "A Velocity-Dependent Model for Needle Insertion in Soft Tissue" MICCAI 2005; LNCS 3750 pp. 624-632, Dated: 2005.

McLellan et al. "Vessel Sealing for Hemostasis During Pelvic Surgery" Int'l Federation of Gynecology and Obstetrics FIGO World Congress 2000, Washington, D.C.

McLellan et al. "Vessel Sealing for Hemostasis During Gynecologic Surgery" Sales/Product Literature 1999.

U.S. Appl. No. 08/926,869, filed Sep. 10, 1997; inventor: James G. Chandler, Abandoned.

U.S. Appl. No. 09/177,950, filed Oct. 23, 1998; inventor: Randel A. Frazier, abandoned.

U.S. Appl. No. 09/387,883, filed Sep. 1, 1999; inventor: Dale F. Schmaltz, abandoned.

U.S. Appl. No. 09/591,328, filed Jun. 9, 2000; inventor: Thomas P. Ryan, abandoned.

U.S. Appl. No. 12/336,970; filed Dec. 17, 2008; inventor: Paul R. Sremeich, abandoned.

U.S. Appl. No. 14/065,644, filed Oct. 29, 2013; inventor: Reschke, abandoned.

* cited by examiner

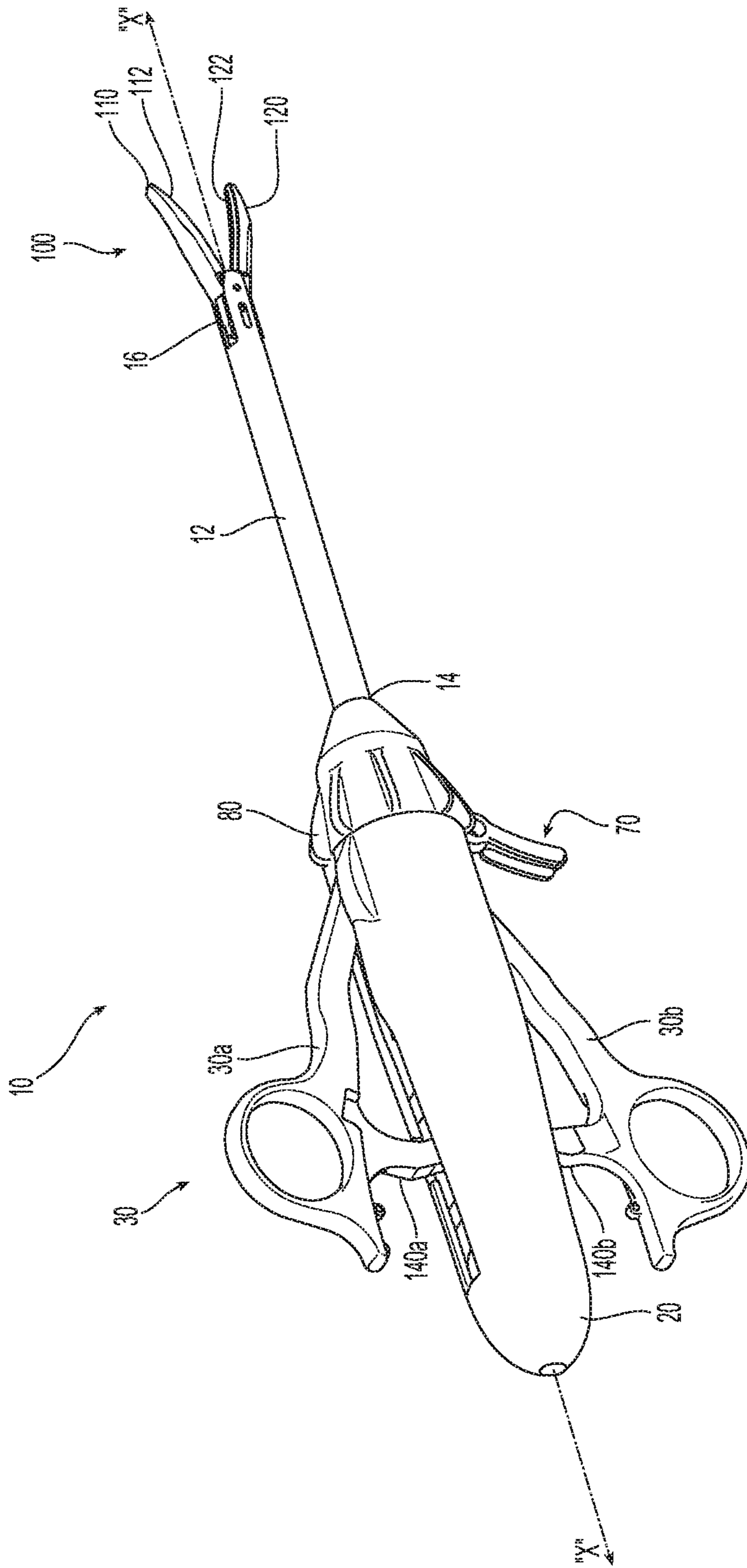


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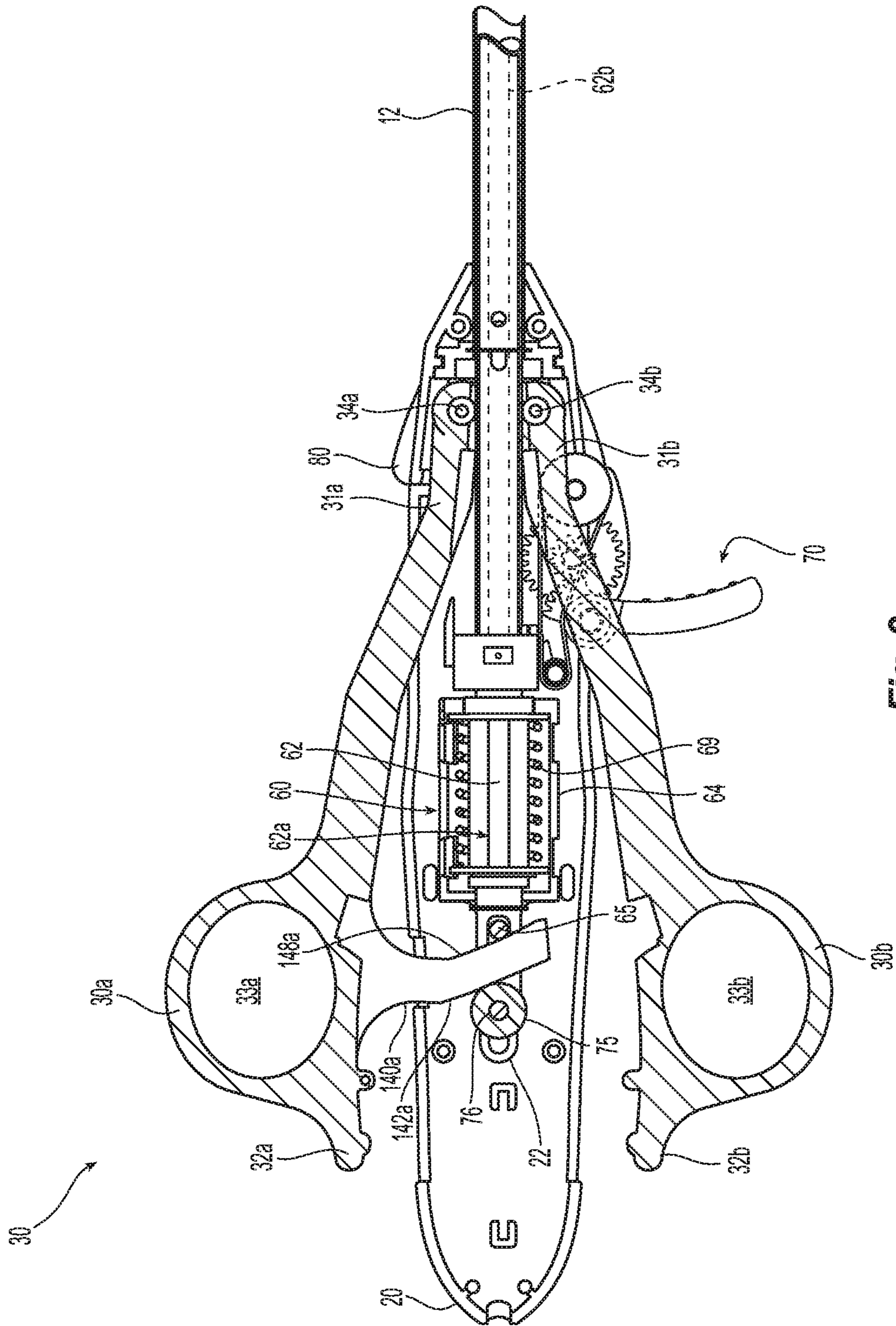


FIG. 2

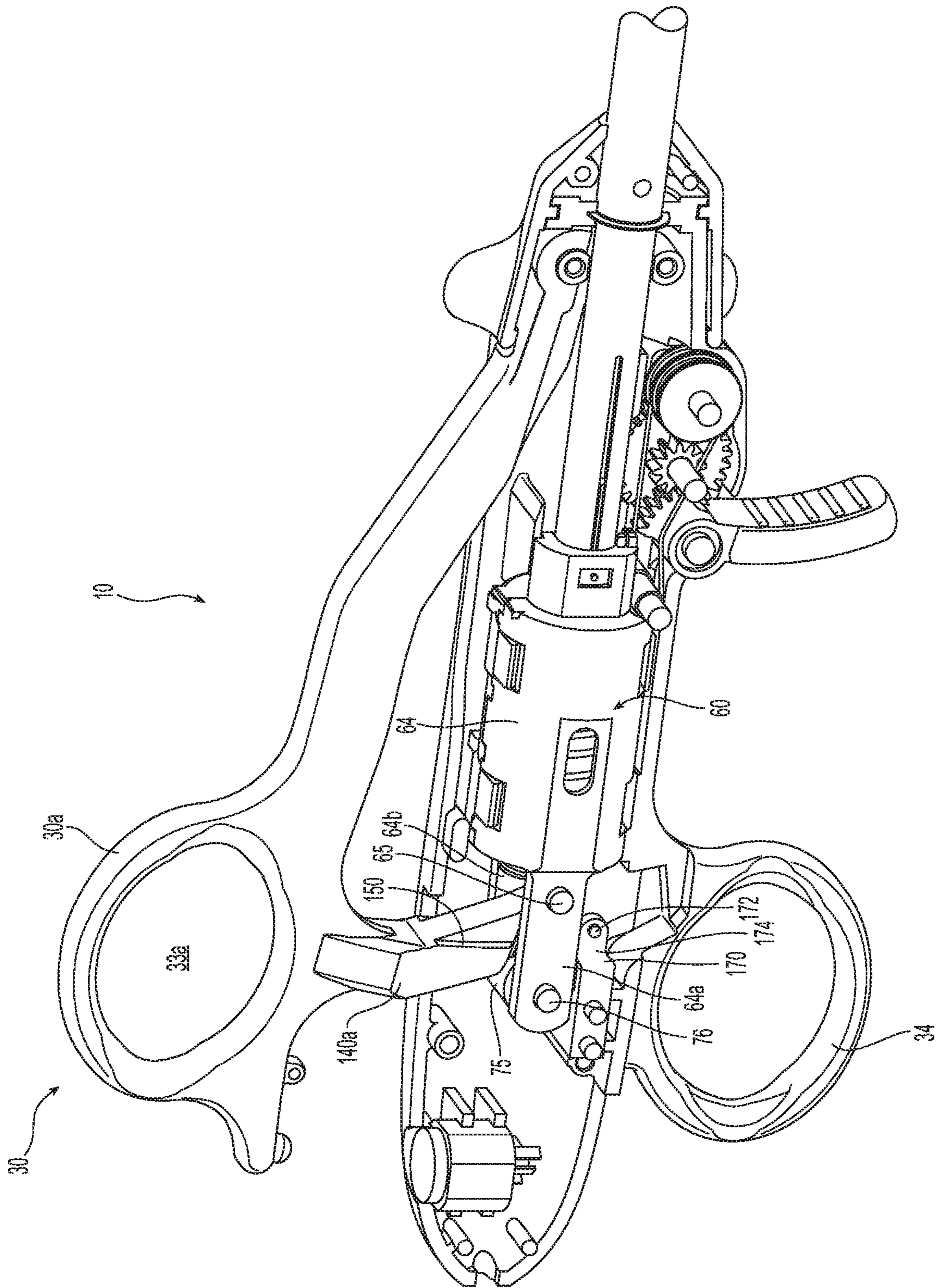


Fig. 3

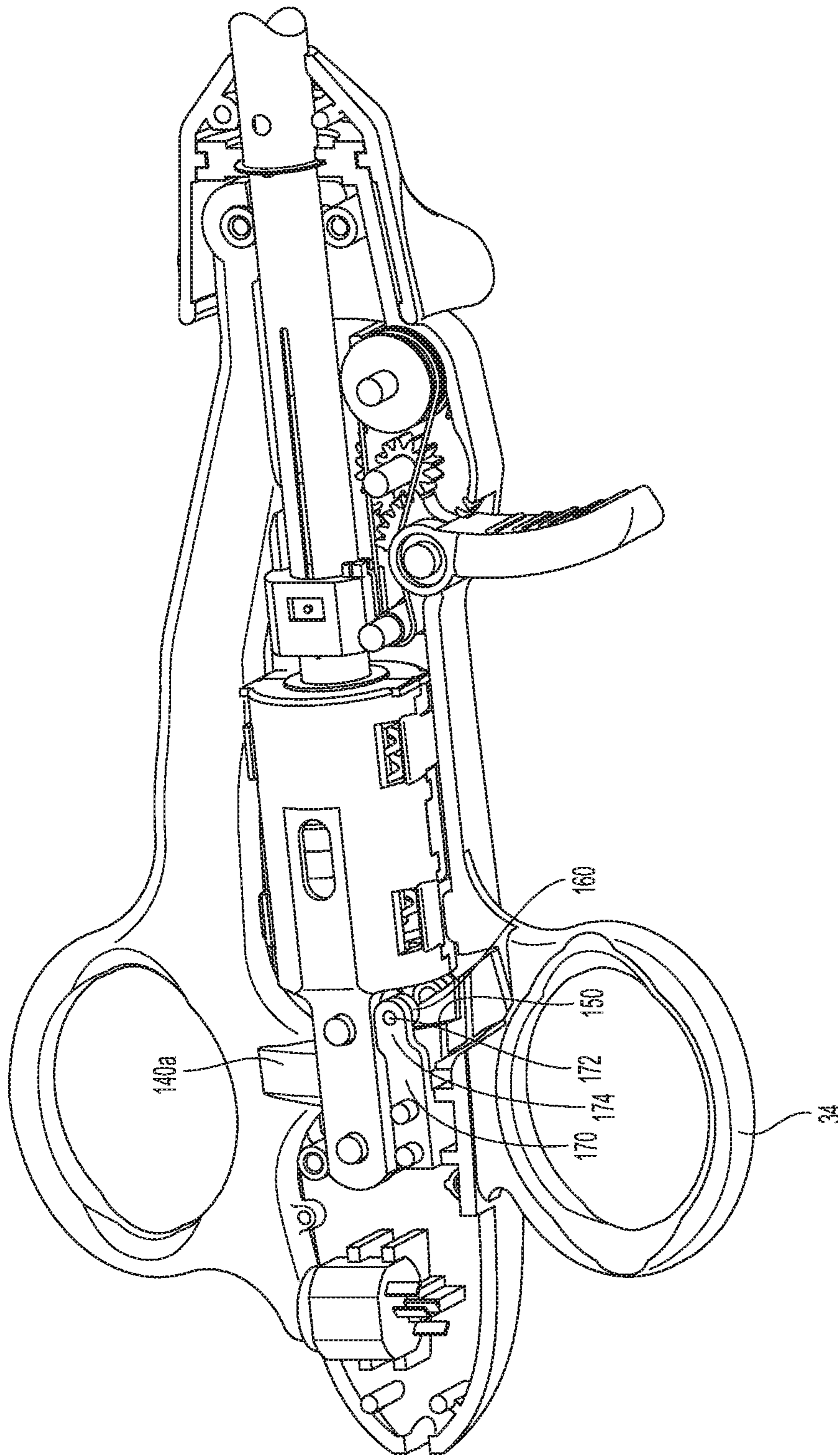


Fig. 4

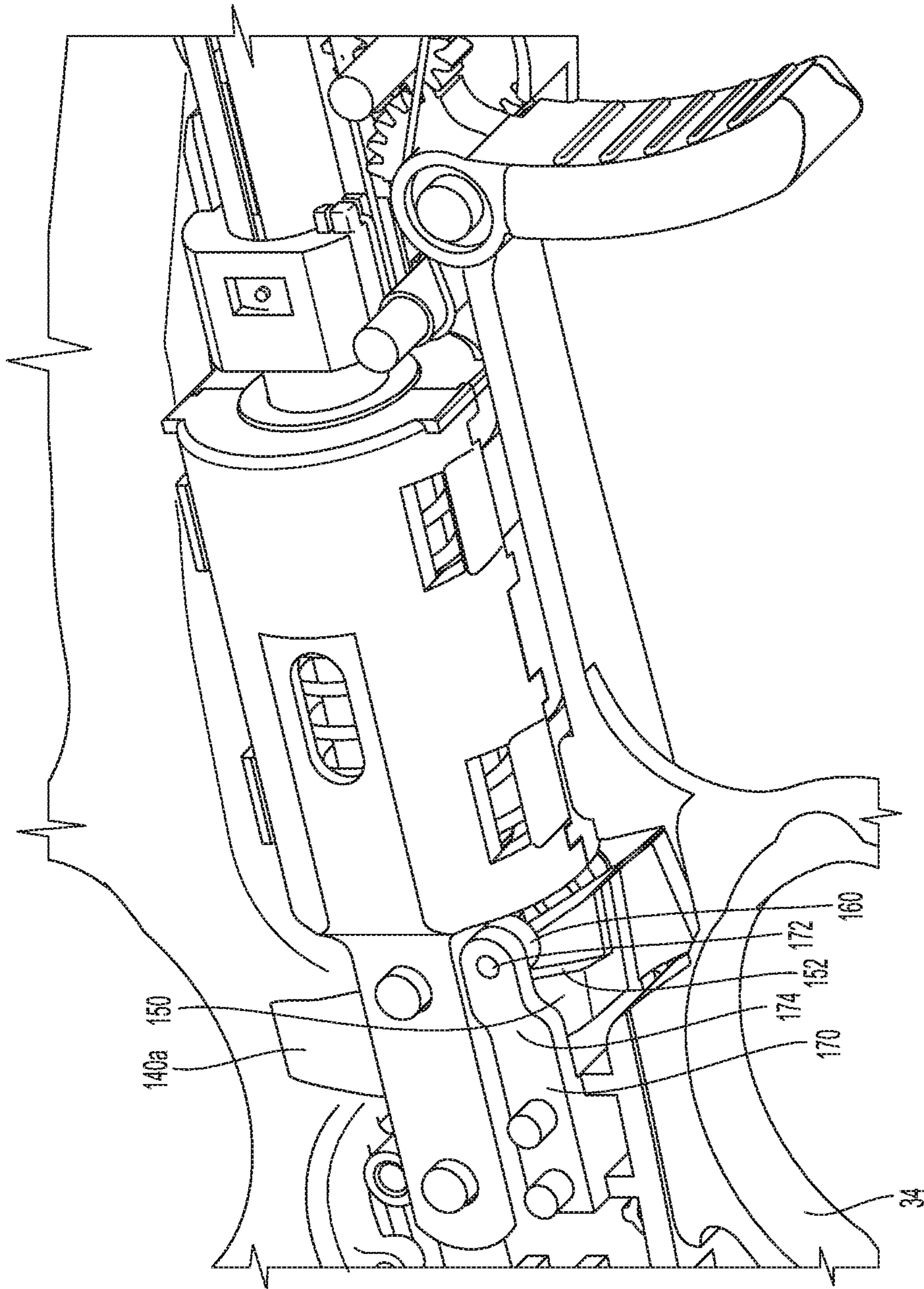


FIG. 5

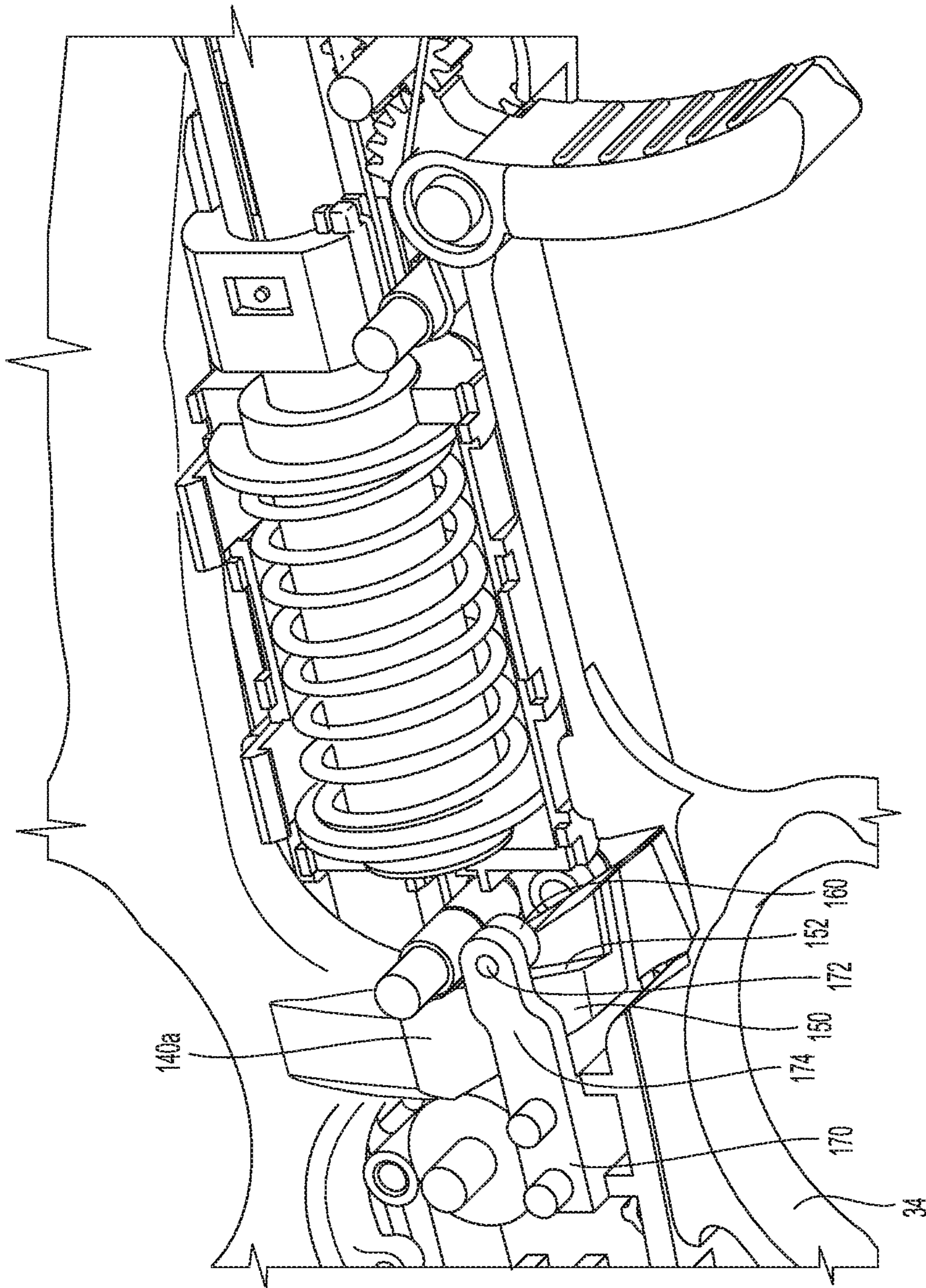


Fig. 6

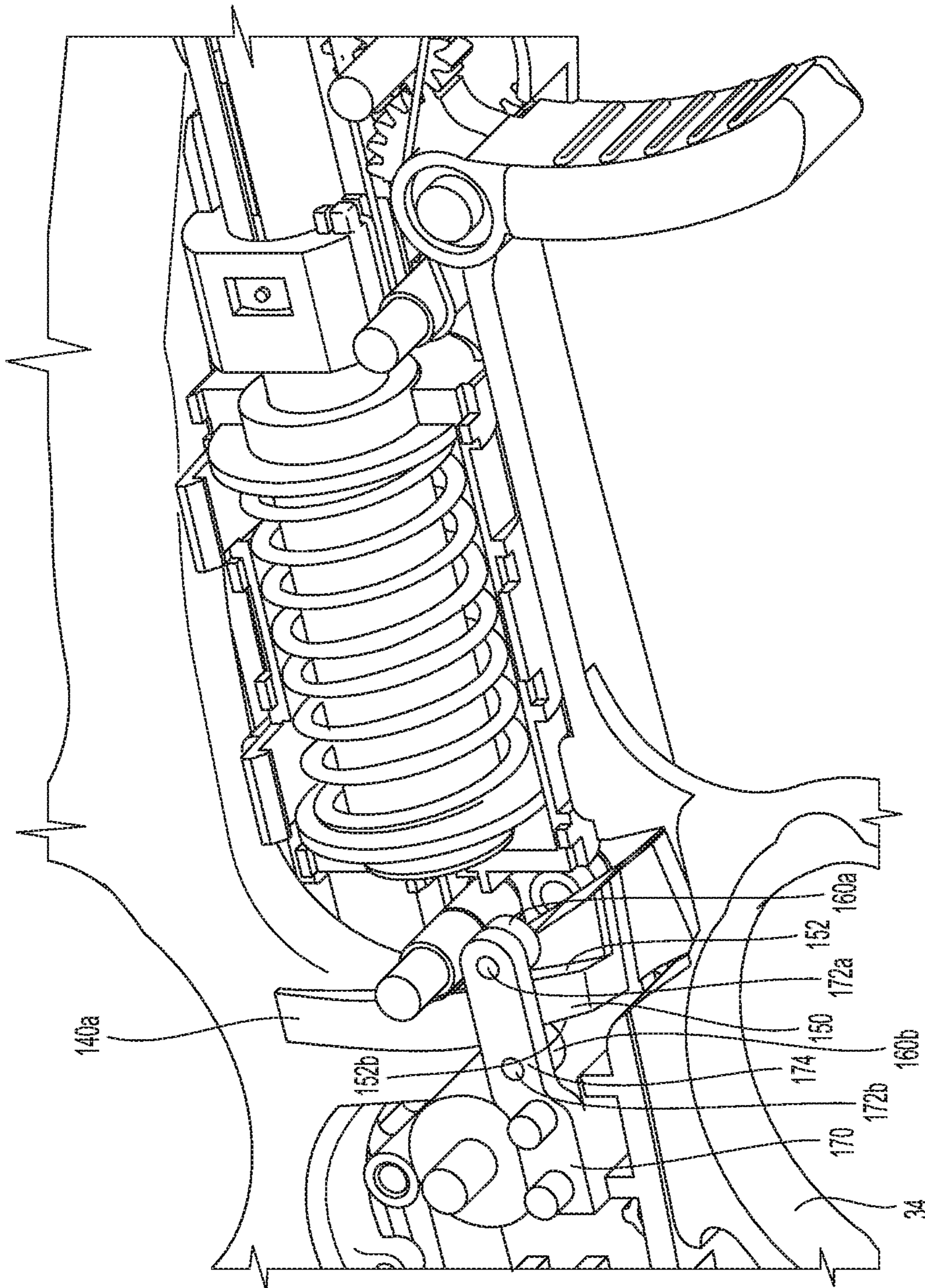


Fig. 6A

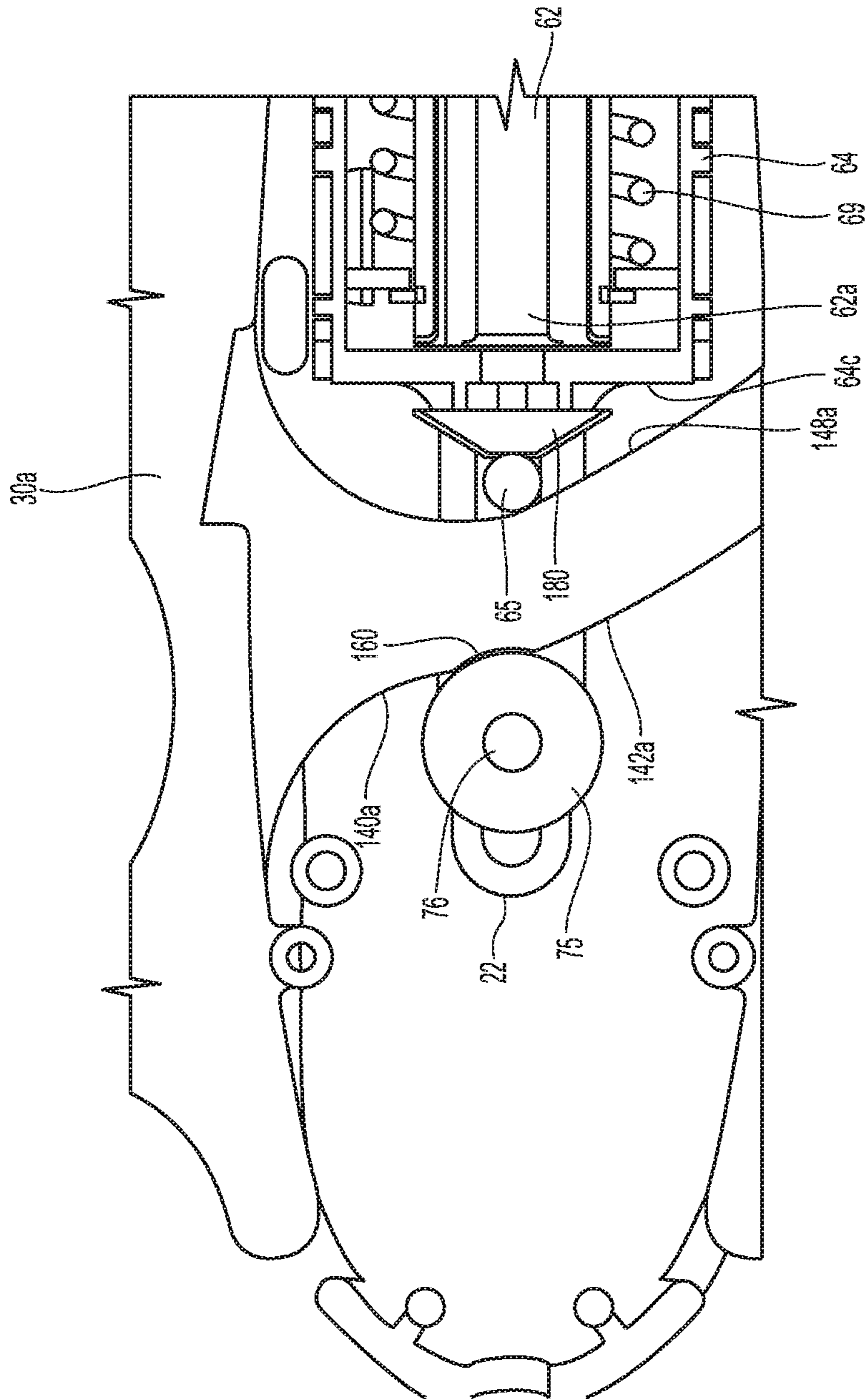


Fig. 7

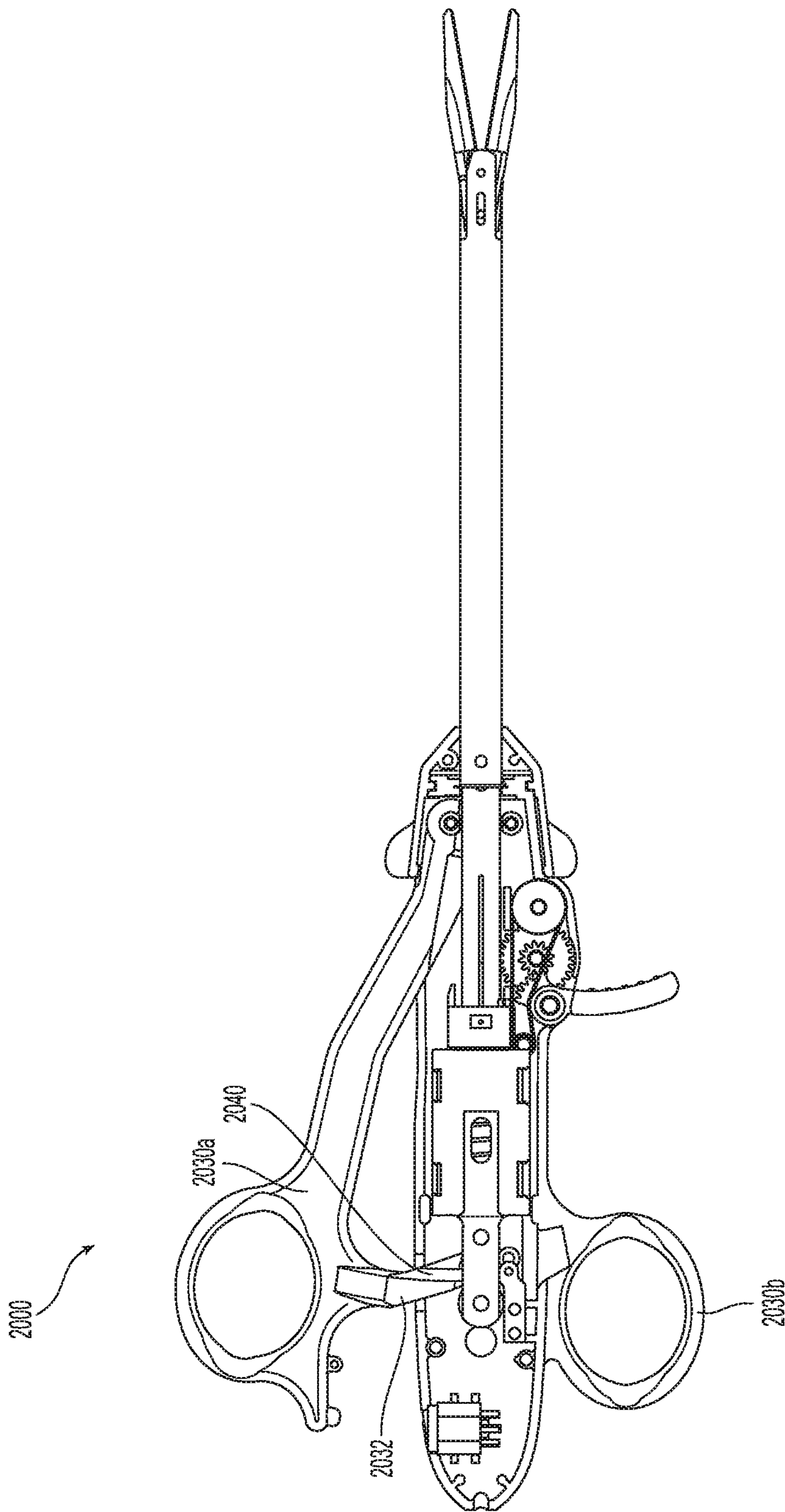


Fig. 8

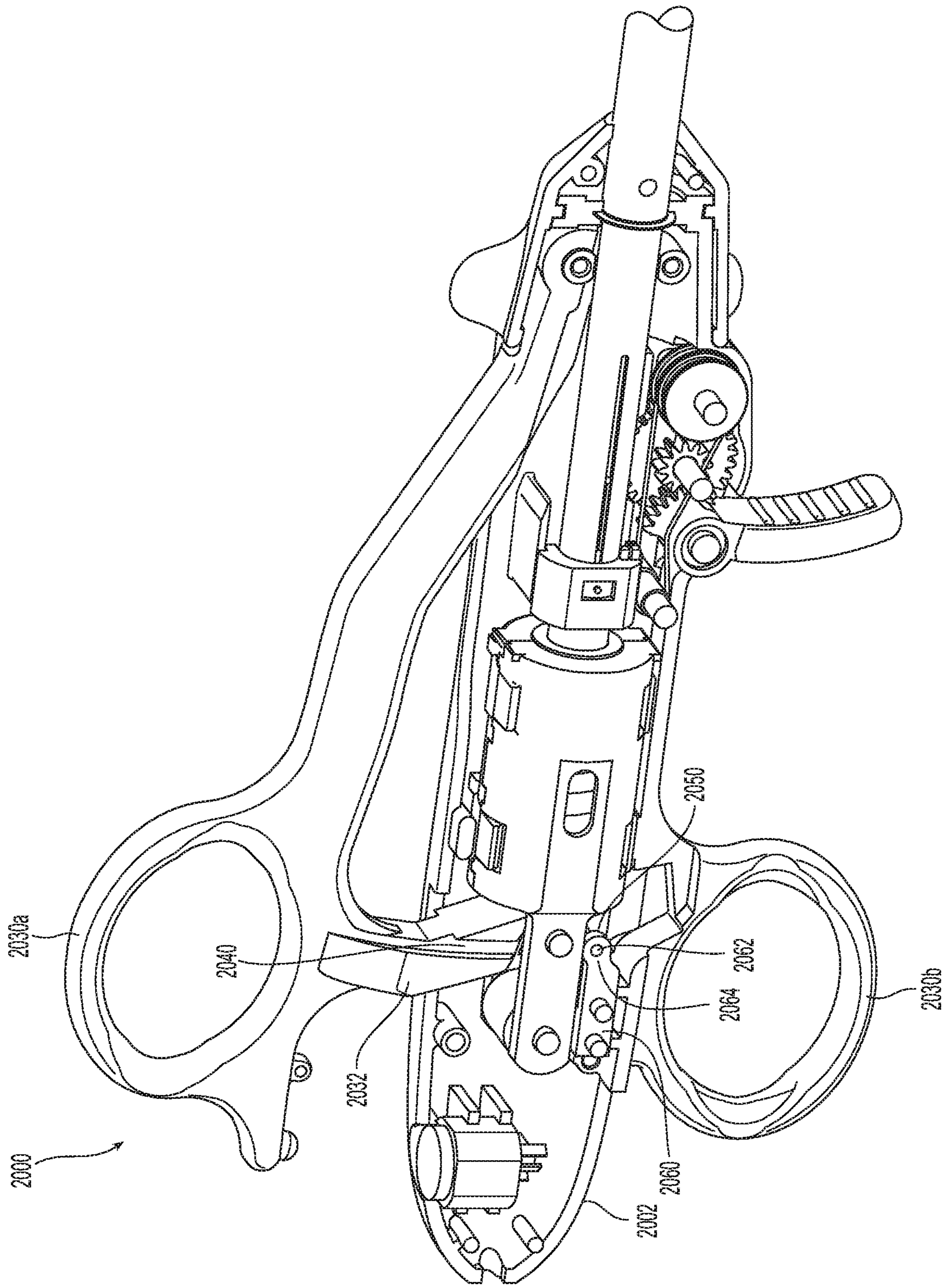


Fig. 9

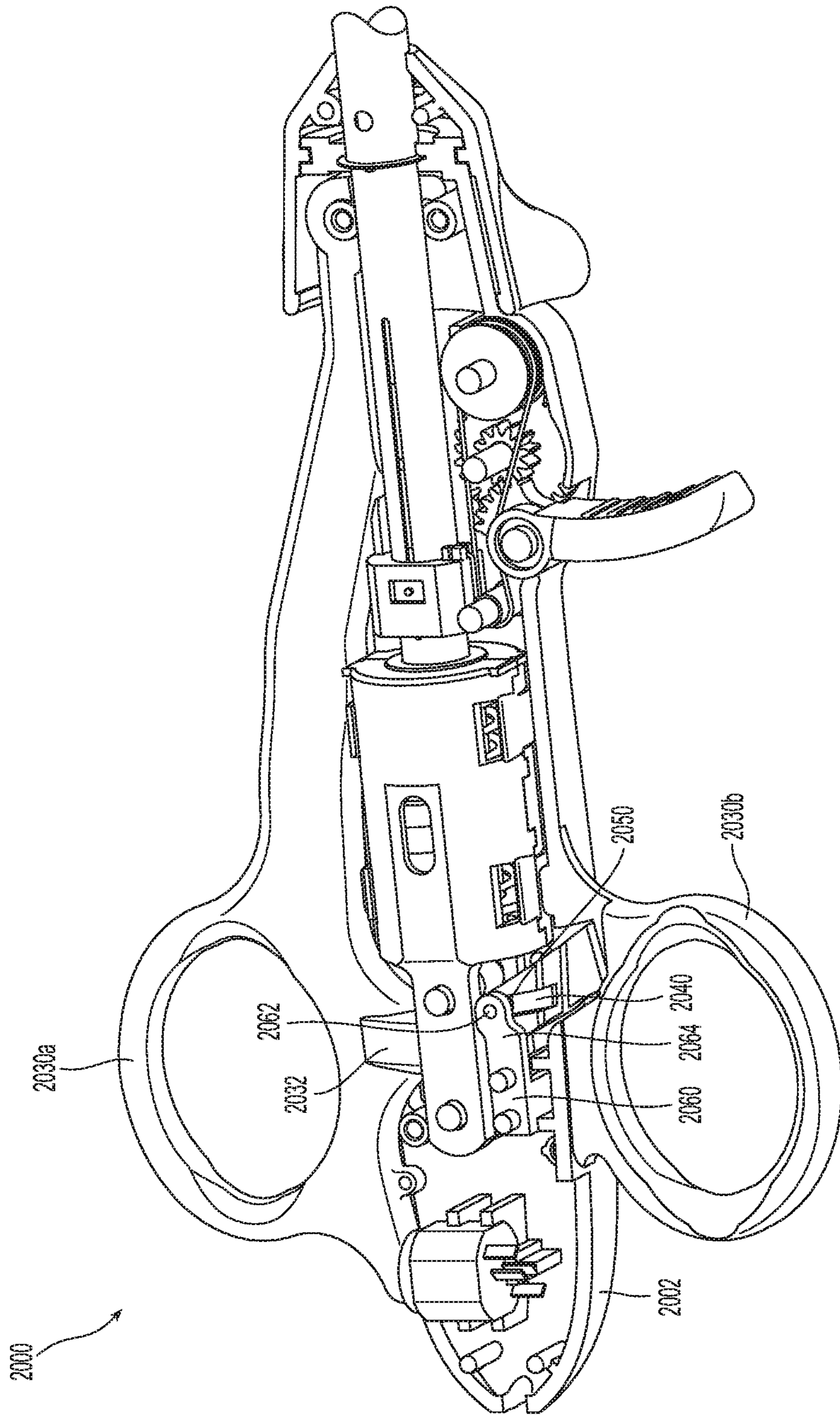


Fig. 10

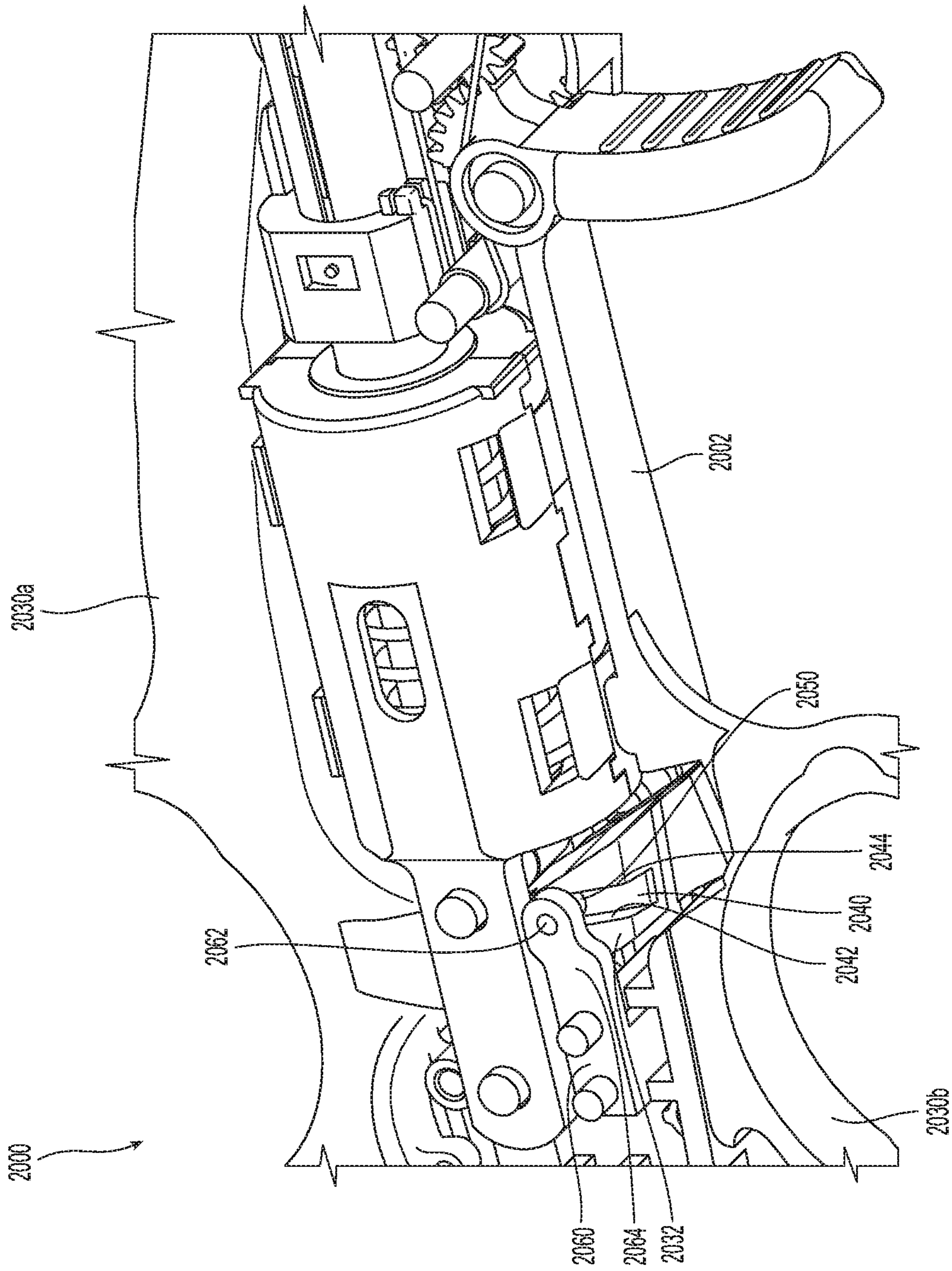


Fig. 11

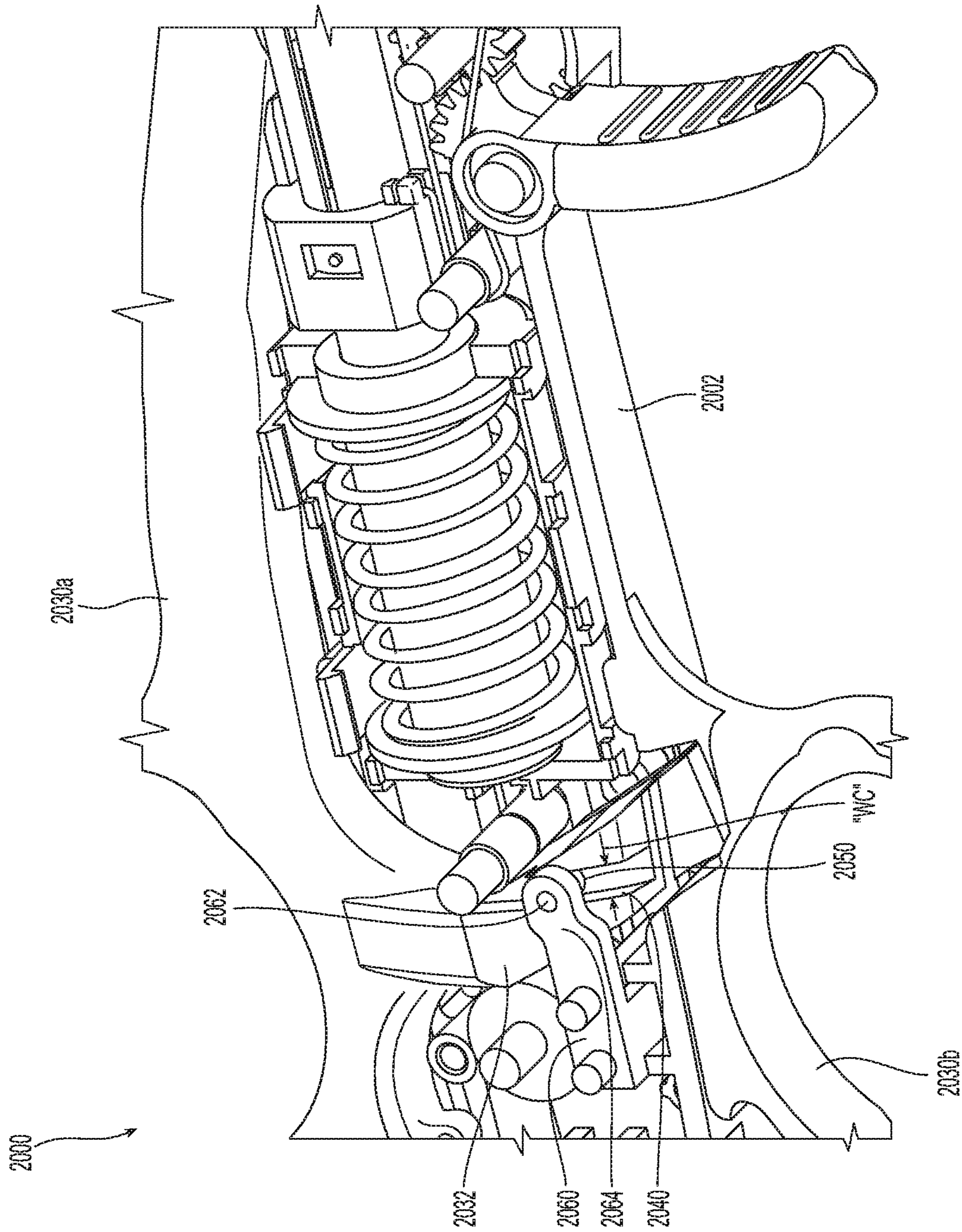


Fig. 12

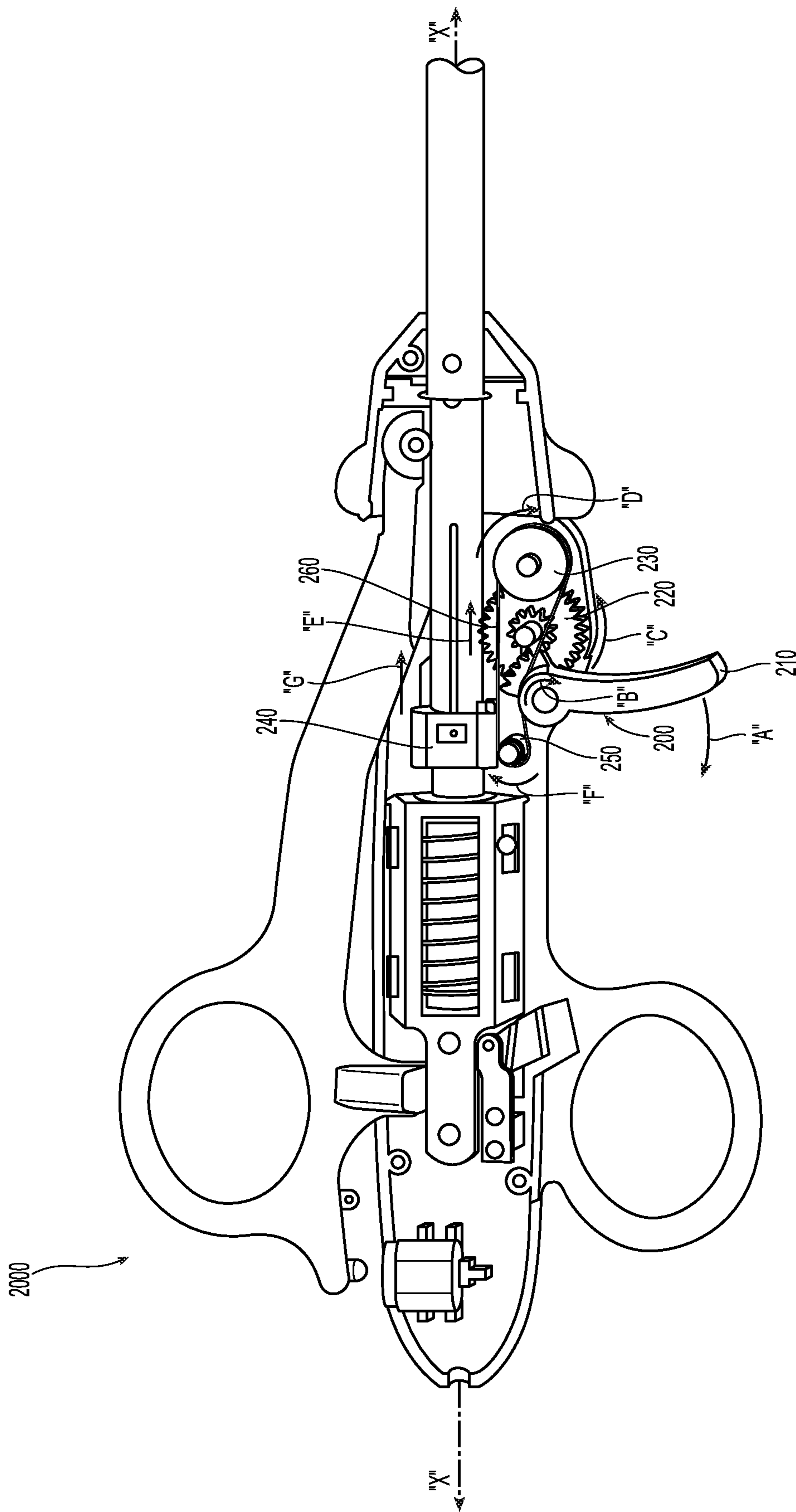


Fig. 13

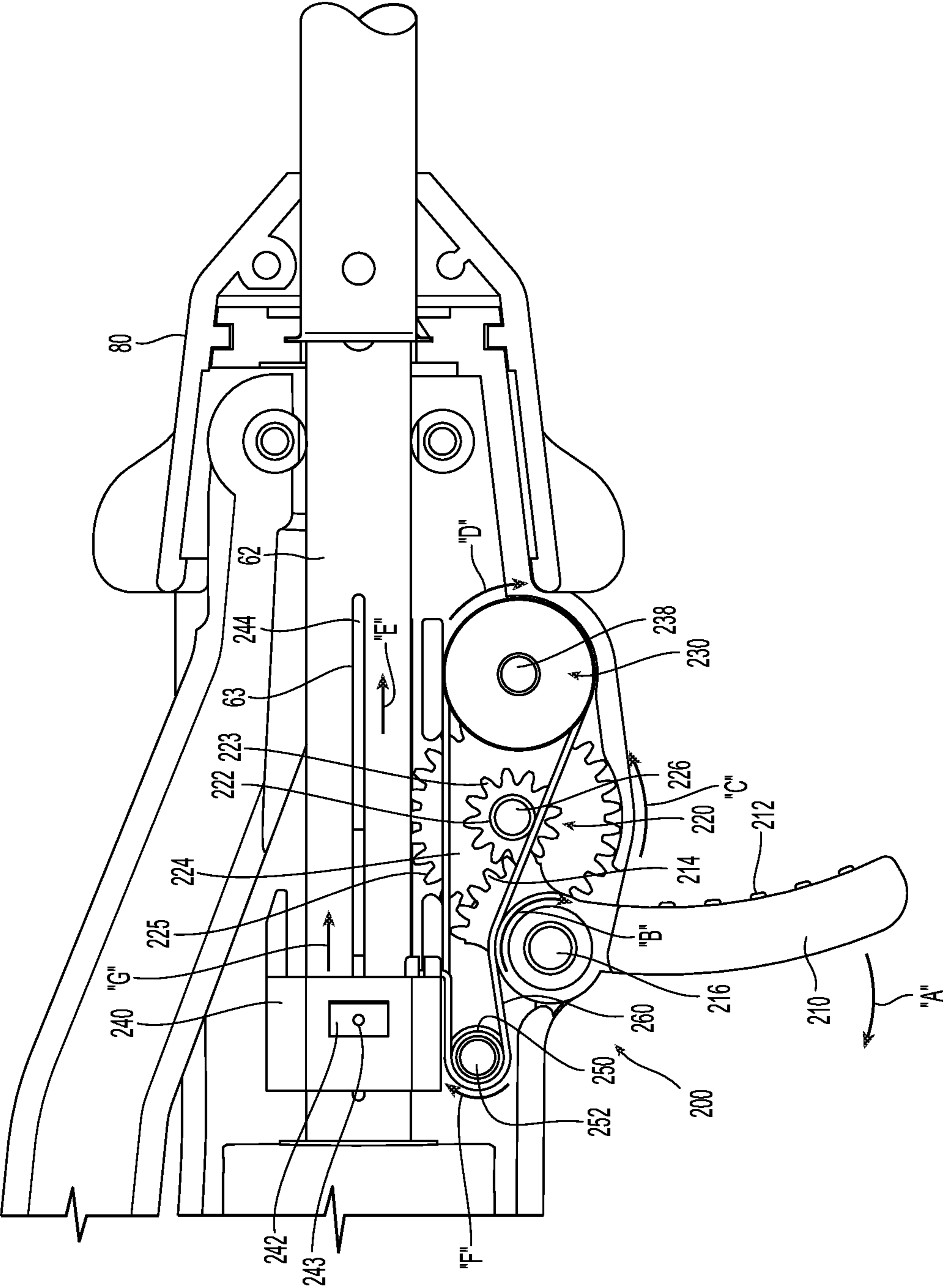


Fig. 14

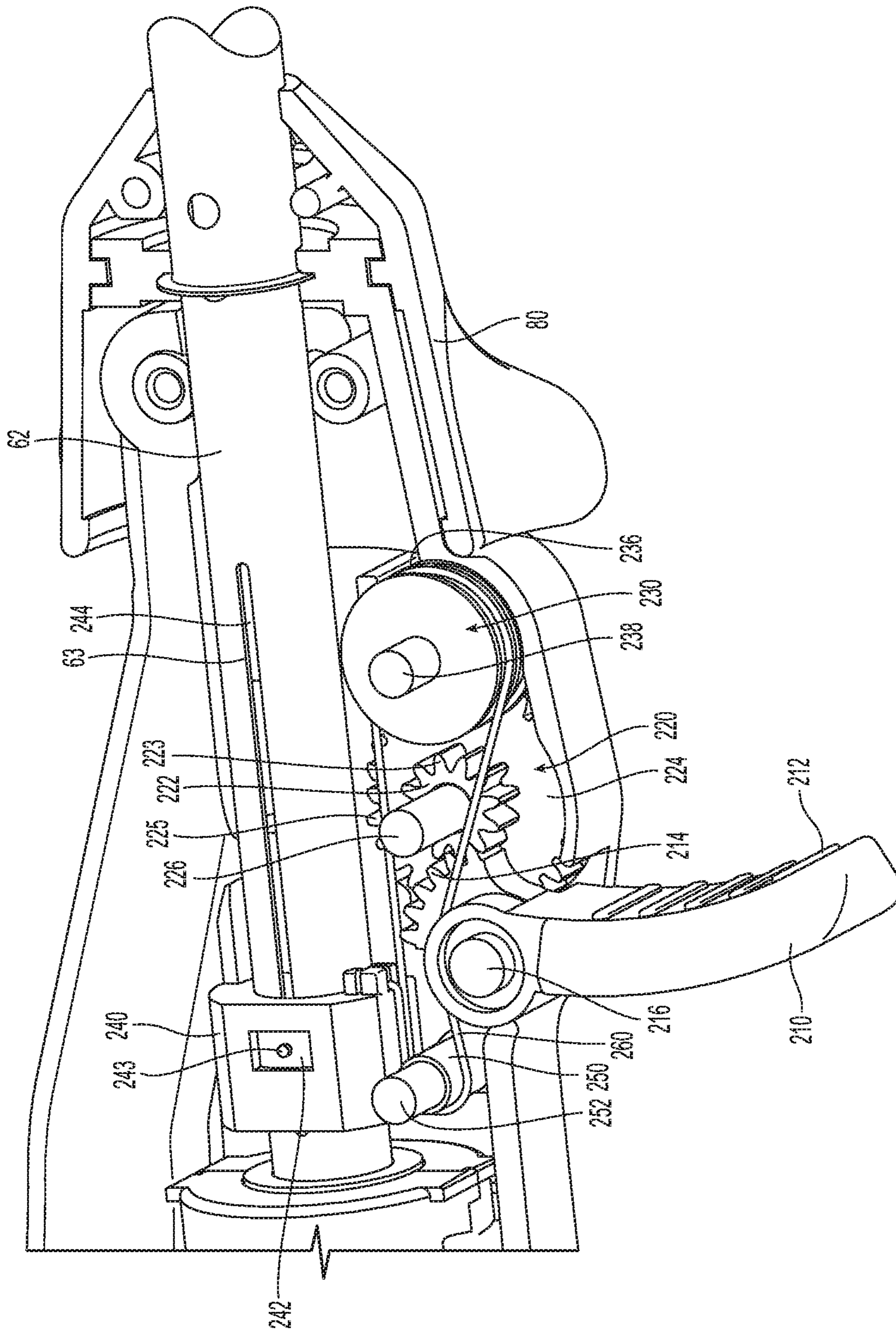


Fig. 15

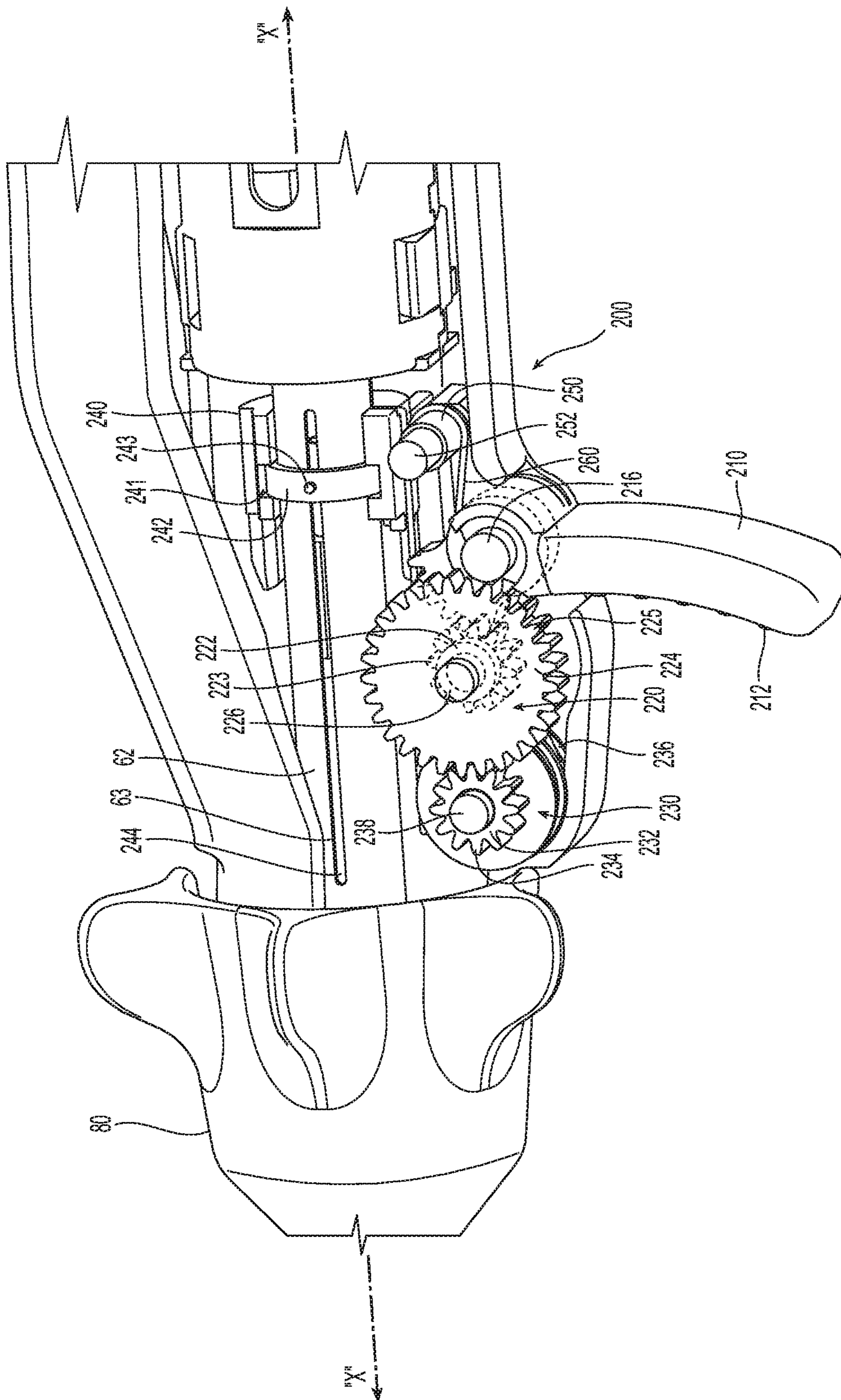


Fig. 16

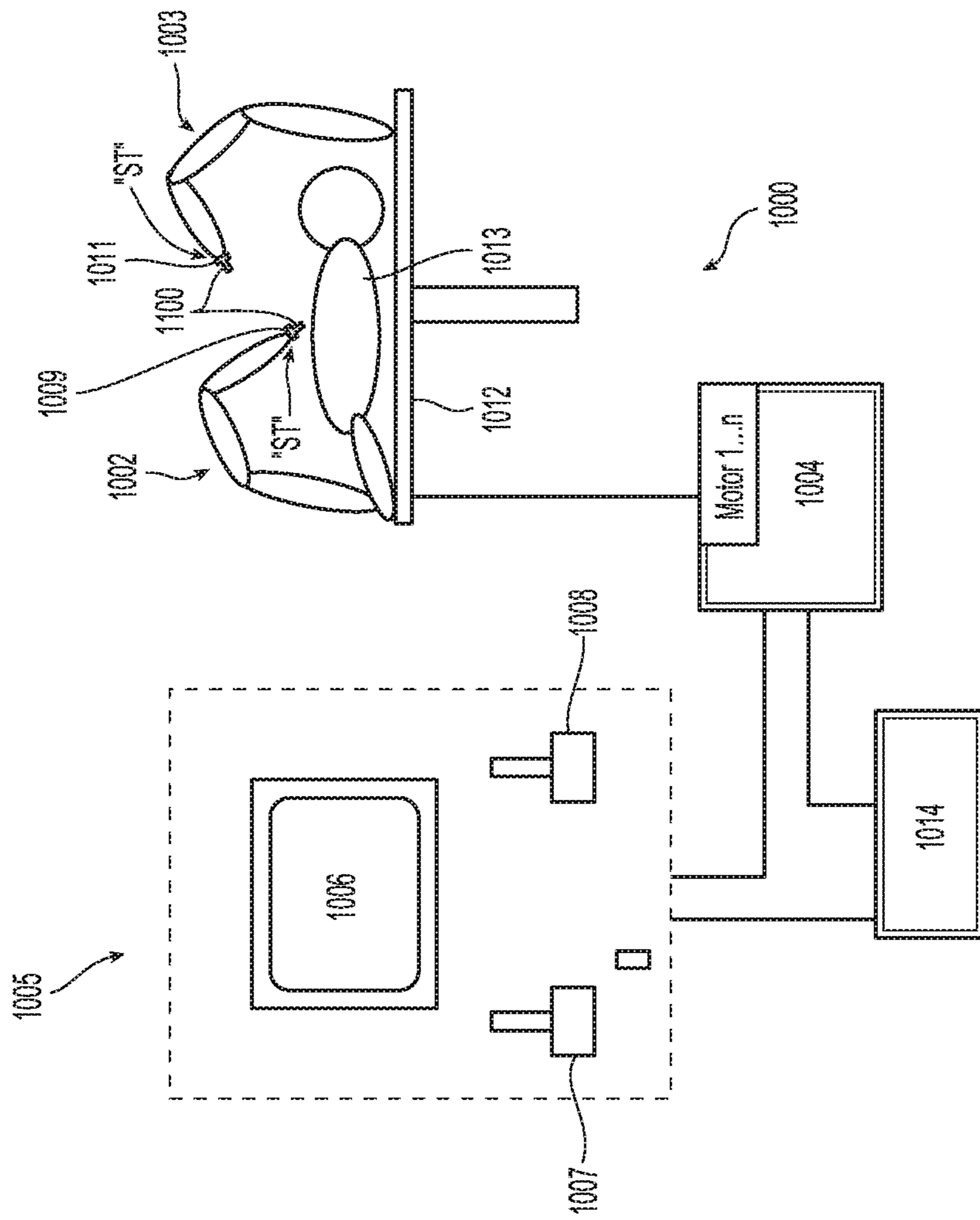


Fig. 17

1**SURGICAL FORCEPS****CROSS REFERENCE TO RELATED APPLICATION**

The present application claims the benefit of and priority to U.S. Provisional Application Ser. No. 62/376,434, filed on Aug. 18, 2016 the entire contents of which are incorporated herein by reference.

BACKGROUND**Technical Field**

The present disclosure relates to surgical forceps and, more particularly, to an endoscopic surgical forceps configured for treating and/or cutting tissue.

Background of Related Art

A surgical forceps is a pliers-like device which relies on mechanical action between its jaw members to grasp, clamp, and constrict tissue. Typically, at least one handle or lever is used to open and close the jaw members, and to provide compression force on tissue between the jaw members, to lock the jaw members in a closed position, and/or to apply energy to the jaw members to seal the tissue disposed therebetween.

Generally, such handles and levers used on surgical instruments are one of two types. One type is a simple pivoted handle that provides a near constant mechanical advantage throughout its stroke, and which is useful in many surgical situations. The second type of handle includes an additional link to provide a geometrically increasing mechanical advantage toward the end of its stroke to help provide the force necessary to compress tissue.

Both of these types of handles fix the mechanical advantage of the drive system such that the drive system cannot be optimized independently over the entire lever stroke. Often times, it may be desirable for a system to include fine dissection capability (a relatively large amount of handle travel for a relatively small amount of jaw member movement) when the jaw members are in an initial, or open position, and to include a high mechanical advantage while applying compression force to tissue disposed between the jaw members when the jaw members are in or near their approximated position (to help reduce surgeon fatigue, for instance). However, current handles are generally unable to achieve both of these desires in a single system.

SUMMARY

The present disclosure relates to a surgical instrument including a housing, an elongated shaft extending distally from the housing and defining a longitudinal axis, an end effector assembly, and a trigger assembly. The end effector assembly is disposed adjacent a distal end of the elongated shaft, and includes a first jaw member and a second jaw member. One or both of the jaw members is movable with respect to the other jaw member from a spaced-apart position to a position closer to the other jaw member for grasping tissue. The trigger assembly is disposed in mechanical cooperation with the housing and is configured to longitudinally translate a drive member. The trigger assembly includes a trigger, a gear assembly, a spool, a slider, and a flexible drive member. The trigger is disposed in mechanical cooperation with the gear assembly. The flexible drive

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member is configured to engage the gear assembly, the spool, and the slider. Movement of the trigger with respect to the housing results in movement of the flexible drive member with respect to the housing and longitudinal movement of the slider with respect to the housing.

In aspects of the present disclosure, the surgical instrument further includes a drive assembly disposed at least partially within the housing. The drive assembly includes a drive bar extending at least partially through the elongated shaft such that longitudinal translation of the drive bar causes the jaw members to move between the spaced-apart position and the closer position for grasping tissue.

In other aspects, the drive bar is rotatable about the longitudinal axis with respect to the housing. In yet other aspects, the drive bar is rotatable about the longitudinal axis with respect to the slider.

In still other aspects, the trigger assembly further includes a ring. The ring is rotationally supported by the slider. In aspects of the present disclosure, the ring is rotationally fixed with respect to the drive bar. In other aspects, the ring is longitudinally translatable with respect to the drive bar.

In yet other aspects, the drive member is longitudinally translatable with respect to the drive bar. In still other aspects, the drive bar is rotatable with respect to the drive member.

In aspects of the present disclosure, the gear assembly includes a first gear and a second gear. The first gear is configured to engage the trigger, and the second gear is configured to engage the spool.

The present disclosure also relates to a trigger assembly for use with a surgical instrument. The trigger assembly includes a trigger, a gear assembly disposed in mechanical cooperation with the trigger, a spool, a slider, and a flexible drive member. The flexible drive member is configured to engage the gear assembly, the spool, and the slider. Actuation of the trigger results in movement of the flexible drive member with respect to the spool and longitudinal movement of the slider with respect to the spool.

In aspects of the present disclosure, the trigger assembly includes a ring rotationally supported by the slider. In other aspects, the ring is longitudinally translatable with respect to the spool.

In still other aspects, the gear assembly includes a first gear and a second gear. The first gear is configured to engage the trigger, and the second gear is configured to engage the spool. In yet other aspects, the first gear and the second gear are rotationally fixed with respect to each other.

In aspects of the present disclosure, the flexible drive member is in contact with the spool and the slider.

In other aspects, the spool includes a spool gear having a plurality of teeth configured to engage a portion of the gear assembly.

BRIEF DESCRIPTION OF THE DRAWINGS

Various aspects of the present disclosure are described herein with reference to the drawings wherein like reference numerals identify similar or identical elements:

FIG. 1 is a perspective view of a surgical forceps provided in accordance with the present disclosure;

FIG. 2 is a sectional view of a handle assembly of the surgical forceps of FIG. 1 where a first cam of a first handle is shown, and where a second cam of a second handle is omitted;

FIGS. 3-6 are perspective views of internal components of the handle assembly of FIGS. 1 and 2;

FIG. 6A is a perspective view of internal components of a handle assembly according to an embodiment of the present disclosure;

FIG. 7 is a sectional view of internal components of the handle assembly of FIGS. 1-6;

FIG. 8 is a sectional view of another embodiment of a surgical forceps provided in accordance with the present disclosure;

FIGS. 9-12 are perspective views of internal components of a handle assembly of the surgical forceps of FIG. 8;

FIG. 13 is a sectional view of a handle assembly of another embodiment of a surgical forceps provided in accordance with the present disclosure;

FIG. 14 is a sectional view of a trigger assembly of the surgical forceps of FIG. 13;

FIGS. 15 and 16 are perspective views of the trigger assembly of the surgical forceps of FIGS. 13-14; and

FIG. 17 is a schematic illustration of a surgical system in accordance with the present disclosure.

DETAILED DESCRIPTION

Embodiments of the presently disclosed surgical forceps are described in detail with reference to the drawings, in which like reference numerals designate identical or corresponding elements in each of the several views. As used herein the term “distal” refers to that portion of the surgical forceps that is farther from the user, while the term “proximal” refers to that portion of the surgical forceps that is closer to the user.

With initial reference to FIG. 1, an embodiment of a surgical forceps in accordance with the present disclosure is shown generally identified by reference character 10. Although surgical forceps 10 is shown configured for use in connection with endoscopic surgical procedures, the present disclosure is equally applicable for surgical instruments used in open surgical procedures and in connection with any suitable surgical instrument. For the purposes herein, forceps 10 is generally described.

Forceps 10 is adapted for use in various surgical procedures and generally includes a housing 20, a handle assembly 30, a trigger assembly 70, a rotating assembly 80, and an end effector assembly 100. Jaw members 110 and 120 of end effector assembly 100 mutually cooperate to grasp, treat, seal and/or cut tissue. Forceps 10 further includes a shaft 12 having a distal end 16 that mechanically engages end effector assembly 100, and a proximal end 14 that mechanically engages housing 20. Forceps 10 may be configured to connect to a source of energy, e.g., a generator (not shown), forceps 10 may be configured as a battery powered instrument, or forceps 10 may be manually powered (e.g., when providing electrosurgical energy is not desired).

As shown in FIGS. 1 and 2, for example, handle assembly 30 includes a first movable handle 30a and a second movable 30b disposed on opposite sides of housing 20. Handles 30a and 30b are movable relative to one another to actuate end effector assembly 100, as will be described in greater detail below. Further, while two movable handles 30a and 30b are shown and described herein, the present disclosure also includes handle assembly 30 including a single movable handle, as shown in FIGS. 3-16, for example. Here, in addition to the single movable handle, a finger loop 34 is included on the opposite side of housing 20 as the single movable handle. Additionally, handle 30b may include the same, mirror-image, or corresponding features as handle 30a.

Rotating assembly 80 is mechanically coupled to housing 20 and is rotatable in either direction, to rotate shaft 12 and, thus, end effector assembly 100 about a longitudinal axis “X” defined by shaft 12. Such a configuration allows end effector assembly 100 to be rotated in either direction with respect to housing 20.

Handle(s) 30a and/or 30b of handle assembly 30 ultimately connect to a drive assembly 60 disposed within housing 20 and that extends through shaft 12 which, together, cooperate to impart movement of jaw members 110 and 120 from an open position wherein jaw members 110 and 120 are disposed in spaced relation relative to one another, to a closed or approximated position wherein jaw members 110 and 120 cooperate to grasp tissue therebetween.

Handles 30a and 30b of handle assembly 30 each include a finger loop or an aperture 33a and 33b, respectively, defined therein which enables a user to grasp and move handles 30a and 30b relative to one another and relative to housing 20 between a spaced-apart position and an approximated position. In the embodiment where handle assembly 30 includes two handles 30a and 30b, each handle 30a and 30b is pivotably coupled to housing 20 at its respective distal end 31a, 31b via pivot pins 34a, 34b, respectively, and extends proximally to proximal ends 32a, 32b, respectively, thereof. As mentioned above, handles 30a, 30b are coupled to drive assembly 60 such that pivoting of handles 30a, 30b about pivot pins 34a, 34b, respectively, and relative to one another effects pivoting of jaw members 110, 120 between the open and closed positions, as discussed in further detail below. In the embodiment where handle assembly 30 includes a single movable handle 30a and a finger loop 34, handle 30a is pivotably coupled to housing at its distal end 31a via pivot pin 34b. Here, movement of handle 30a with respect to housing 20 effects pivoting of jaw members 110, 120 between the open and closed positions.

With particular reference to FIG. 2, drive assembly 60 includes a drive bar 62 defining a proximal end 62a disposed within housing 20 and a distal end 62b that extends through shaft 12, ultimately coupling to jaw members 110, 120. A mandrel 64 disposed within housing 20 is engaged with the proximal end 62a of drive bar 62. Mandrel 64 is slidably engaged with at least one track 22 (see FIG. 2) defined within housing 20 to guide longitudinal translation of mandrel 64 and, thus, drive bar 62, relative to housing 20. Other suitable guide/alignment mechanisms are also contemplated. A spring 69 is positioned within mandrel 64 and is configured to prevent over compression of tissue when jaw members 110, 120 are in the closed or approximated position.

A follower 75 is rotatably supported by an axle 76, which extends through a bore of follower 75. Axle 76 is supported (e.g., rotatably supported) by proximal extensions 64a, 64b of mandrel 64. A cam follower (e.g., a pin within a sleeve) 65 is also supported (e.g., rotatably supported) by proximal extensions 64a, 64b of mandrel 64.

While the following description discusses the use of two handles 30a, 30b, the use of a single handle 30a may also be utilized without departing from the scope of the present disclosure. In order to move jaw members 110, 120 from the open position to the closed position, handles 30a and/or 30b are squeezed, e.g., pivoted about pivot pins 34a, 34b, inwardly towards one another and housing 20. As handle(s) 30a, 30b are pivoted in this manner, proximal ends 32a, 32b of handles 30a, 30b are approximated relative to housing 20 and one another. The approximation of proximal ends 32a, 32b of handles 30a, 30b towards one another causes exten-

sions **140a**, **140b** of respective handles **30a**, **30b** to urge follower **75**, mandrel **64** and drive bar **62** proximally, thus approximating jaw members **110**, **120**. Movement of handles **30a**, **30b** toward their open position causes extensions **140a**, **140b** to urge cam follower **65**, mandrel **64** and drive bar **62** distally, thus causing jaw members **110**, **120** to move toward their open position, as further described below. The spring force of spring **69** may be configured such that jaw members **110**, **120** impart a closure force between jaws within a range of about 3 kg/cm² to about 16 kg/cm², although other closure forces are also contemplated.

Additionally, with reference to FIGS. 3-6, extension **140a** includes a rib **150** thereon. The shape of rib **150** is arcuate when used with a pivoting handle **30a**; rib **150** may be linear when used with a non-pivoting handle (not shown). Rib **150** is configured to be contacted by a roller **160**.

As shown in FIGS. 4-6, roller **160** is supported by a support **170**. Support **170** is fixed to housing **20** of surgical forceps **10** and includes a pin **172** extending through a leg **174** of support **170**. Pin **172** rotationally supports roller **160**. Roller **160** is longitudinally fixed with respect to housing **20** and is configured to engage rib **150** of extension **140a**.

As handle **30a**, and thus extension **140a**, is moved, roller **160** moves along rib **150**. More particularly, as handle **30a** is moved, roller **160** contacts and thus supports a distal wall **152** of rib **150**. For example, when handle **30a** is moved generally downward (as viewed in FIG. 3) to approximate the jaw members, for instance, roller **160** contacts distal wall **152** of rib **150**. Thus, roller **160** provides support to rib **150**, and thus handle **30a**, during approximation of jaw members, e.g., to restrict or minimize unintended bending or flexing motion in extension **140a**, handle **30a**, and other features within housing **20**.

An alternate embodiment is shown in FIG. 6A, which includes a first roller **160a** and a second roller **160b**. Each of first roller **160a** and second roller **160b** is supported by support **170**. Support **170** is fixed to housing **20** of surgical forceps **10** and includes a first pin **172a** and a second pin **172b** extending through leg **174** of support **170**. First pin **172a** rotationally supports first roller **160a**, and second pin **172b** rotationally supports second roller **160b**. First and second rollers **160a**, **160b** are longitudinally fixed with respect to housing **20** and are configured to engage rib **150** of extension **140a**.

As handle **30a**, and thus extension **140a**, is moved, first and second rollers **160a**, **160b** move along rib **150**. More particularly, as handle **30a** is moved, first roller **160a** contacts and thus supports distal wall **152** of rib **150**. For example, when handle **30a** is moved generally downward (as viewed in FIG. 3) to approximate the jaw members, for instance, first roller **160a** contacts distal wall **152** of rib **150**. Thus, first roller **160a** provides support to rib **150**, and thus handle **30a**, during approximation of jaw members, e.g., to restrict or minimize unintended bending or flexing motion in extension **140a**, handle **30a**, and other features within housing **20**. Additionally, when handle **30a** is moved generally upward (as viewed in FIG. 3) to open the jaw members, for instance, second roller **160b** contacts a proximal wall **152b** of rib **150**. Thus, second roller **160b** provides support to rib **150**, and thus handle **30a**, during opening of jaw members, e.g., to restrict or minimize unintended bending or flexing motion in extension **140a**, handle **30a**, and other features within housing **20**.

During use, a surgeon may desire fine (vs. gross) control of jaw members **110**, **120** during some stages of use. For example, the surgeon may wish to have greater control of the movement of the jaw members **110**, **120** during dissection of

tissue, manipulation of tissue, and precise placement of jaw members **110**, **120** about target tissue. For such fine control of jaw members **110**, **120**, a relative large amount of travel of handles **30a**, **30b** (or a single handle) would correspond to a relative small amount of travel of jaw members **110**, **120**. Some surgeons may also desire to have a high mechanical advantage during other stages of use. For example, a surgeon may wish to utilize a high mechanical advantage while applying compression force to tissue. To achieve such a high mechanical advantage, a relative small amount of travel of handles **30a**, **30b** would correspond to a relative large amount of travel of jaw members **110**, **120**. Typically, surgical instruments only allow for either fine control of jaw members **110**, **120** or a high mechanical advantage. Examples of one surgical forceps configured to allow both fine control of jaw members and a high mechanical advantage at different stages of the actuation stroke of handles is described in U.S. Provisional Patent Application Ser. No. 62/247,279, filed on Oct. 28, 2015, the entire contents of which is incorporated by reference herein.

With particular reference to FIG. 7, to help ensure that contact is maintained between follower **75** and a proximal cam surface **142a**, and between cam follower **65** and a distal cam surface **148a** (e.g., to account for manufacturing tolerances, and/or to allow greater manufacturing tolerances, thus reducing costs), surgical forceps **10** may include an engagement spring **180** disposed between a proximal wall **64c** of mandrel **64** and cam follower **65**. Engagement spring **180** is configured to urge cam follower **65** proximally toward and into contact with distal cam surface **148a**. Engagement spring **180** may be cone-like (e.g., frusto-conical) in shape, or a so-called Belleville washer.

With particular reference to FIGS. 8-12, an additional embodiment of surgical forceps is shown and is indicated by reference character **2000**. Surgical forceps **2000** is similar to surgical forceps **10** discussed above and only the differences are discussed in detail herein.

Surgical forceps **2000** includes a movable handle **2030a** and a finger loop **2030b**. In lieu of finger loop **2030b**, surgical forceps **2000** may include a second movable handle. Handle **2030a** includes an extension **2032** having a groove or channel **2040** defined therein. A roller **2050** is movably positioned within channel **2040**.

More particularly, channel **2040** extends within extension **2032** of handle **2030a** and is defined by a proximal wall **2042** and a distal wall **2044** (FIG. 11). The shape of channel **2040** is arcuate when used with a pivoting handle **2030a**; channel **2040** may be linear when used with a non-pivoting handle (not shown). Channel **2040** includes a width "wc" (FIG. 12) which may be uniform along its entire length or which may vary along at least a portion of its length.

Roller **2050** is supported by a support **2060**. Support **2060** is fixed to housing **2002** of surgical forceps **2000** and includes a pin **2062** extending through a leg **2064** of support **2060**. Pin **2062** rotationally supports roller **2050**. Roller **2050** is longitudinally fixed with respect to housing **2002** and is configured to engage channel **2040** of extension **2032**. Roller **2050** includes a width in the longitudinal direction. The width of roller **2050** is smaller than width "wc" of channel **2040**, thus enabling roller **2050** to move within channel **2040**.

As handle **2030a**, and thus extension **2032**, is moved, roller **2050** moves within channel **2040**. More particularly, as handle **2030a** is moved, roller **2050** contacts proximal wall **2042** and distal wall **2044** of channel **2040**. For example, when handle **2030a** is moved generally downward (as viewed in FIG. 8) to approximate the jaw members, for

instance, roller **2050** may contact distal wall **2044** of channel **2040**; when handle **2030a** is moved generally upward (as viewed in FIG. **8**) to move the jaw members to the open position, for example, roller **2050** may contact proximal wall **2042** of channel **2040**. Thus, channel **2040** provides support to roller **2050** at all times during manipulation of the jaw members, e.g., to restrict or minimize unintended bending motion.

The difference between the width of roller **2050** and the width “wc” of channel **2040** determines the amount of travel or “play” that handle **2030a** can undergo while being actuated; a small difference between these distances results in a lower amount of “play.”

Surgical forceps **10**, **2000** may also include features to help maintain the handle(s) in the closed position, and may include features for providing feedback to the user at certain stages of approximating or opening the jaw members. Such features are described in U.S. Provisional Patent Application Ser. No. 62/247,279, filed on Oct. 28, 2015, the entire contents of which have been incorporated by reference hereinabove.

The present disclosure also includes methods of manipulating jaw members **110**, **120** using fine and gross controls, as described above. For example, disclosed methods include moving handle **30a**, **30b** of surgical instrument **10** from a non-actuated position a first distance to an intermediate position to cause first jaw member **110** to move a first amount, and moving handle **30a**, **30b** from the intermediate position a second distance to a fully actuated position to cause first jaw member **110** to move a second amount. Here, the first distance is the same as the second distance, and the first amount is less than the second amount, thus resulting in an initial fine movement of jaw member **110**, and a subsequent gross movement of jaw member **110**.

With particular reference to FIGS. **13-16**, details of a second type of trigger assembly **200** are shown. Trigger assembly **200** of this embodiment includes a trigger **210**, a gear assembly **220**, a drive spool **230**, a knife slider **240**, a roller **250**, and a flexible drive member **260**. As discussed below, actuation of trigger assembly **200** is configured to longitudinally translate a drive member (e.g., a knife drive shaft **244**). Additionally, while trigger assembly **200** is shown used in connection with a particular surgical forceps **2000**, trigger assembly **200** may also be used in connection with surgical forceps **10**, or an additional type of surgical device.

With particular reference to FIGS. **14** and **15**, trigger **210** includes an actuation portion **212** configured for direct engagement by the user (e.g., physician), a plurality of trigger teeth **214**, and is rotatable about a trigger pin **216**. Gear assembly **220** (e.g., a cluster gear) includes a first gear **222** having a plurality of teeth **223**, and a second gear **224** having a plurality of teeth **225**. First gear **222** and second gear **224** are rotationally fixed with respect to each other, and are rotatable about a gear pin **226**.

Drive spool **230** includes a spool gear **232** having a plurality of teeth **234** (see FIG. **16**), and spool portion **236**. Drive spool **230** is rotatable about a spool pin **238**. A knife ring **242** is rotationally disposed within a portion of knife slider **240**. Knife ring **242** is rotatable about the longitudinal axis “X” with respect to knife slider **240**. Roller **250** is rotatable about a roller pin **252**. Flexible drive member **260** is in contact with spool portion **236** of drive spool **230**, knife slider **240**, and roller **250**. Flexible drive member **260** can be made from any suitable material such as nylon, a para-aramid synthetic fiber (e.g., Kevlar®), high-modulus polyethylene (HMPE), etc. for example. Flexible drive member

260 can also be made from plastic, e.g., having a rectangular cross-section (such as a zip-tie). In such embodiments, the pushing of various elements may be facilitated due to the strength of plastic. Additionally, assembly of surgical forceps **2000** may be facilitated using a plastic flexible drive member **260**, for example, as fewer loops may be necessary to accomplish each desired action (e.g., proximal and distal translation of knife slider **240**).

Details regarding the various interactions between the components of trigger assembly **200** are discussed herein with continued reference to FIGS. **13-16**. Trigger teeth **214** of trigger **210** engage or mesh with teeth **223** of first gear **222** of gear assembly **220**. Accordingly, movement of actuation portion **212** in the general direction of arrow “A” in FIGS. **13** and **14** causes rotation of trigger teeth **214** about trigger pin **216** in the general direction of arrow “B” in FIGS. **13** and **14**, which causes rotation of first gear **222** about gear pin **226** in the general direction of arrow “C” in FIGS. **13** and **14**.

First gear **222** of gear assembly **220** is rotationally fixed with respect to second gear **224** of gear assembly **220**. Teeth **225** of second gear **224** of gear assembly **220** engage or mesh with teeth **234** of spool gear **232** of drive spool **230**. Accordingly, rotation of first gear **222** about gear pin **226** in the general direction of arrow “C” causes rotation of second gear **224** about gear pin **226** in the general direction of arrow “C,” which causes rotation of spool gear **232** and drive spool **230** about spool pin **238** in the general direction of arrow “D” in FIGS. **13** and **14**. Spool portion **236** of drive spool **230** is rotationally fixed with respect to spool gear **232**, such that rotation of spool gear **232** causes a corresponding rotation of drive spool **230**.

Flexible drive member **260** extends at least partially around spool portion **236** of drive spool **230**, extends at least partially around roller **250**, and is engaged with (e.g., wrapped around) a portion of knife slider **240**. Flexible drive member **260** is longitudinally fixed with respect to knife slider **240**. Accordingly, rotation of spool portion **236** of drive spool **230** in the general direction of arrow “D” causes translation of flexible drive member **260** in the general direction of arrow “E” in FIGS. **13** and **14**, which causes roller **250** to rotate about roller pin **252** in the general direction of arrow “F” in FIGS. **13** and **14**. Additionally, based on the way flexible drive member **260** engages a portion of knife slider **240** (as shown in FIG. **15**), translation of flexible drive member **260** in the general direction of arrow “E” causes knife slider **240** to move in the general direction of arrow “G” (or distally) in FIGS. **13** and **14**.

Further, and with continued reference to FIG. **16**, knife slider **240** includes a cutout **241** that rotationally supports knife ring **242**, such that knife ring **242** is rotatable about the longitudinal axis “X” with respect to knife slider **240** and with respect to trigger **210**, for example. Additionally, knife ring **242** is pinned to a knife drive shaft **244** and to drive bar **62** by a ring pin **243**, such that rotation of rotating assembly **80** causes rotation of drive bar **62** and knife ring **242** about the longitudinal axis “X” with respect to knife slider **240**. Moreover, ring pin **243** extends through a longitudinal slot **63** of drive bar **62**. Thus, longitudinal translation of knife slider **240** causes a corresponding longitudinal translation of knife ring **242** and knife drive shaft **244**.

Accordingly, actuation of trigger **210** in a first direction (e.g., in the general direction of arrow “A”) causes rotation of gear assembly **220**, rotation of drive spool **230**, movement of flexible drive member **260** around spool portion **236** of drive spool **230** and around roller **250**, which causes distal translation or advancement of knife slider **240**, knife ring

242 and knife drive shaft 244 to cut tissue, for example. Additionally, movement of trigger 210 in a second direction (e.g., in the general opposite direction of arrow "A") causes proximal translation or retraction of knife drive shaft 244.

Additionally, while the illustrated embodiments depict one type of surgical instrument (i.e., surgical forceps), the present disclosure includes the use of various features described herein in connection with other types of surgical devices including at least one pivotable handle or lever. For instance, various handle assemblies for actuating handle(s) and corresponding drive assemblies are contemplated for translating drive bar 62 and are discussed in commonly-owned U.S. Pat. No. 7,857,812, the entire contents of which are incorporated by reference herein.

Additionally, further details of a surgical forceps having a similar handle assembly to the disclosed handle assembly 30 are disclosed in U.S. Pat. No. 8,430,876, the entire contents of which being incorporated by reference herein. Further details of an electrosurgical instrument are disclosed in U.S. Pat. Nos. 7,101,371 and 7,083,618, the entire contents of which being incorporated by reference herein.

The various embodiments disclosed herein may also be configured to work with robotic surgical systems and what is commonly referred to as "Telesurgery." Such systems employ various robotic elements to assist the surgeon and allow remote operation (or partial remote operation) of surgical instrumentation. Various robotic arms, gears, cams, pulleys, electric and mechanical motors, etc. may be employed for this purpose and may be designed with a robotic surgical system to assist the surgeon during the course of an operation or treatment. Such robotic systems may include remotely steerable systems, automatically flexible surgical systems, remotely flexible surgical systems, remotely articulating surgical systems, wireless surgical systems, modular or selectively configurable remotely operated surgical systems, etc.

The robotic surgical systems may be employed with one or more consoles that are next to the operating theater or located in a remote location. In this instance, one team of surgeons or nurses may prepare the patient for surgery and configure the robotic surgical system with one or more of the surgical instruments disclosed herein while another surgeon (or group of surgeons) remotely controls the instrument(s) via the robotic surgical system. As can be appreciated, a highly skilled surgeon may perform multiple operations in multiple locations without leaving his/her remote console which can be both economically advantageous and a benefit to the patient or a series of patients.

The robotic arms of the surgical system are typically coupled to a pair of master handles by a controller. The handles can be moved by the surgeon to produce a corresponding movement of the working ends of any type of surgical instrument (e.g., end effectors, graspers, knives, scissors, etc.) which may complement the use of one or more of the embodiments described herein. The movement of the master handles may be scaled so that the working ends have a corresponding movement that is different, smaller or larger, than the movement performed by the operating hands of the surgeon. The scale factor or gearing ratio may be adjustable so that the operator can control the resolution of the working ends of the surgical instrument(s).

The master handles may include various sensors to provide feedback to the surgeon relating to various tissue parameters or conditions, e.g., tissue resistance due to manipulation, cutting or otherwise treating, pressure by the instrument onto the tissue, tissue temperature, tissue impedance, etc. As can be appreciated, such sensors provide the

surgeon with enhanced tactile feedback simulating actual operating conditions. The master handles may also include a variety of different actuators for delicate tissue manipulation or treatment further enhancing the surgeon's ability to mimic actual operating conditions.

With particular reference to FIG. 17, a medical work station is shown generally as work station 1000 and generally may include a plurality of robot arms 1002, 1003; a control device 1004; and an operating console 1005 coupled with control device 1004. Operating console 1005 may include a display device 1006, which may be set up in particular to display three-dimensional images; and manual input devices 1007, 1008, by means of which a person (not shown), for example a surgeon, may be able to telemanipulate robot arms 1002, 1003 in a first operating mode.

Each of the robot arms 1002, 1003 may include a plurality of members, which are connected through joints, and an attaching device 1009, 1011, to which may be attached, for example, a surgical tool "ST" supporting an end effector 1100, in accordance with any one of several embodiments disclosed herein, as will be described in greater detail below.

Robot arms 1002, 1003 may be driven by electric drives (not shown) that are connected to control device 1004. Control device 1004 (e.g., a computer) may be set up to activate the drives, in particular by means of a computer program, in such a way that robot arms 1002, 1003, their attaching devices 1009, 1011 and thus surgical instrument 10 (including end effector 300) execute a desired movement according to a movement defined by means of manual input devices 1007, 1008. Control device 1004 may also be set up in such a way that it regulates the movement of robot arms 1002, 1003 and/or of the drives.

Medical work station 1000 may be configured for use on a patient 1013 lying on a patient table 1012 to be treated in a minimally invasive manner by means of end effector 1100. Medical work station 1000 may also include more than two robot arms 1002, 1003, the additional robot arms likewise being connected to control device 1004 and being telemanipulatable by means of operating console 1005. A medical instrument or surgical tool (including an end effector 1100) may also be attached to the additional robot arm. Medical work station 1000 may include a database 1014, in particular coupled to with control device 1004, in which are stored, for example, pre-operative data from patient/living being 1013 and/or anatomical atlases.

From the foregoing and with reference to the various figure drawings, those skilled in the art will appreciate that certain modifications can also be made to the present disclosure without departing from the scope of the same. While several embodiments of the disclosure have been shown in the drawings, it is not intended that the disclosure be limited thereto, as it is intended that the disclosure be as broad in scope as the art will allow and that the specification be read likewise. Therefore, the above description should not be construed as limiting, but merely as exemplifications of particular embodiments. Those skilled in the art will envision other modifications within the scope and spirit of the claims appended hereto.

What is claimed is:

1. A surgical instrument, comprising:

a housing;

an elongated shaft extending distally from the housing and defining a longitudinal axis;

an end effector assembly disposed adjacent a distal end of the elongated shaft, the end effector assembly including a first jaw member and a second jaw member, at least one of the jaw members movable with respect to the

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other jaw member from a spaced-apart position to a position closer to the other jaw member for grasping tissue; and

a trigger assembly disposed in mechanical cooperation with the housing and configured to longitudinally translate a drive member, the trigger assembly including a trigger, a gear assembly, a spool, a slider, and a flexible drive member, the trigger disposed in mechanical cooperation with the gear assembly, the flexible drive member configured to engage the gear assembly, the spool, and the slider, the flexible drive member configured as a continuous loop, wherein movement of the trigger with respect to the housing results in movement of the flexible drive member with respect to the housing and longitudinal movement of the slider with respect to the housing.

2. The surgical instrument according to claim 1, further comprising a drive assembly disposed at least partially within the housing, the drive assembly including a drive bar extending at least partially through the elongated shaft such that longitudinal translation of the drive bar causes the jaw members to move between the spaced-apart position and the closer position for grasping tissue.

3. The surgical instrument according to claim 2, wherein the drive bar is rotatable about the longitudinal axis with respect to the housing.

4. The surgical instrument according to claim 2, wherein the drive bar is rotatable about the longitudinal axis with respect to the slider.

5. The surgical instrument according to claim 2, wherein the trigger assembly further comprises a ring rotationally supported by the slider.

6. The surgical instrument according to claim 5, wherein the ring is rotationally fixed with respect to the drive bar.

7. The surgical instrument according to claim 6, wherein the ring is longitudinally translatable with respect to the drive bar.

8. The surgical instrument according to claim 5, wherein the ring is rotatable relative to the housing.

9. The surgical instrument according to claim 5, wherein the slider is rotationally fixed relative to the housing.

10. The surgical instrument according to claim 2, wherein the drive member is longitudinally translatable with respect to the drive bar.

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11. The surgical instrument according to claim 10, wherein the drive bar is rotatable with respect to the drive member.

12. The surgical instrument according to claim 1, wherein the gear assembly includes a first gear and a second gear, the first gear configured to engage the trigger, and the second gear configured to engage the spool.

13. A trigger assembly for use with a surgical instrument, the trigger assembly comprising:

a trigger;

a gear assembly disposed in mechanical cooperation with the trigger;

a spool;

a slider; and

a flexible drive member, the flexible drive member configured to engage the gear assembly, the spool, and the slider, wherein actuation of the trigger results in movement of the flexible drive member with respect to the spool and longitudinal movement of the slider with respect to the spool, wherein an amount of contact between the flexible drive member and the spool remains constant during actuation of the trigger.

14. The trigger assembly according to claim 13, further comprising a ring rotationally supported by the slider.

15. The trigger assembly according to claim 14, wherein the ring is longitudinally translatable with respect to the spool.

16. The trigger assembly according to claim 13, wherein the gear assembly includes a first gear and a second gear, the first gear configured to engage the trigger, and the second gear configured to engage the spool.

17. The trigger assembly according to claim 16, wherein the first gear and the second gear are rotationally fixed with respect to each other.

18. The trigger assembly according to claim 13, wherein the flexible drive member is in contact with the spool and the slider.

19. The trigger assembly according to claim 13, wherein the spool includes a spool gear having a plurality of teeth configured to engage a portion of the gear assembly.

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