



US010687887B2

(12) **United States Patent**
Dycus et al.

(10) **Patent No.:** **US 10,687,887 B2**
(45) **Date of Patent:** **Jun. 23, 2020**

(54) **VESSEL SEALER AND DIVIDER**
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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

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(21) Appl. No.: **16/391,210**
(22) Filed: **Apr. 22, 2019**
(65) **Prior Publication Data**
US 2019/0247111 A1 Aug. 15, 2019

Related U.S. Application Data

(63) Continuation of application No. 16/053,052, filed on Aug. 2, 2018, now Pat. No. 10,265,121, which is a (Continued)

(51) **Int. Cl.**
A61B 18/14 (2006.01)
A61B 90/00 (2016.01)
(Continued)

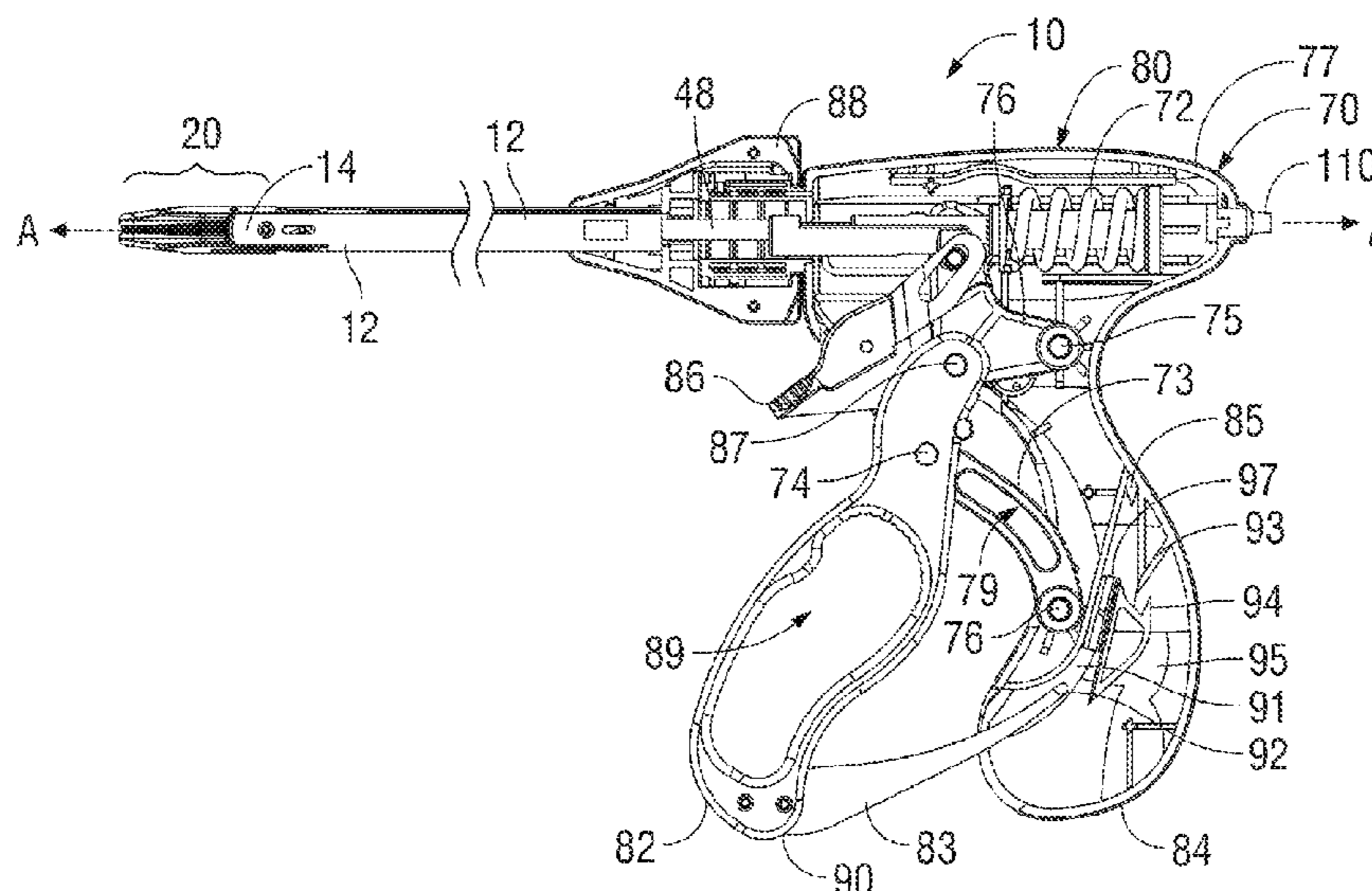
(52) **U.S. Cl.**
CPC **A61B 18/1445** (2013.01); **A61B 18/1482** (2013.01); **A61B 90/03** (2016.02);
(Continued)

(58) **Field of Classification Search**
CPC . A61B 17/32; A61B 18/1206; A61B 18/1445; A61B 18/1482;
(Continued)

(57) **ABSTRACT**

A bipolar forceps includes an elongated shaft having opposing jaw members at a distal end thereof. The jaw members are movable relative to one another from a first position wherein the jaw members are disposed in spaced relation relative to one another to a second position wherein the jaw members cooperate to grasp tissue therebetween. The jaws members are connected to a source of electrical energy such that the jaw members are capable of conducting energy through tissue held therebetween to effect a tissue seal. At least one non-conductive and spaced-apart stop member is disposed on an inner-facing surface of the jaw members to regulate the gap distance between the jaw members when tissue is held therebetween. The forceps also includes a longitudinally reciprocating knife which severs the tissue after sealing at a location which is proximate the sealing site.

13 Claims, 6 Drawing Sheets



Related U.S. Application Data

continuation of application No. 15/911,739, filed on Mar. 5, 2018, now Pat. No. 10,251,696, which is a continuation of application No. 15/338,663, filed on Oct. 31, 2016, now abandoned, which is a continuation of application No. 14/719,887, filed on May 22, 2015, now abandoned, which is a continuation of application No. 13/584,194, filed on Aug. 13, 2012, now abandoned, which is a continuation of application No. 12/348,748, filed on Jan. 5, 2009, now Pat. No. 8,241,284, which is a continuation of application No. 10/471,818, filed as application No. PCT/US01/11413 on Apr. 6, 2001, now Pat. No. 7,473,253.

(51) **Int. Cl.**

A61B 17/32 (2006.01)
A61B 17/29 (2006.01)
A61B 18/00 (2006.01)
A61B 18/12 (2006.01)
A61B 18/18 (2006.01)
A61B 17/00 (2006.01)

(52) **U.S. Cl.**

CPC *A61B 17/32* (2013.01); *A61B 18/1206* (2013.01); *A61B 2017/00539* (2013.01); *A61B 2017/2926* (2013.01); *A61B 2018/0063* (2013.01); *A61B 2018/00077* (2013.01); *A61B 2018/00178* (2013.01); *A61B 2018/00196* (2013.01); *A61B 2018/00404* (2013.01); *A61B 2018/126* (2013.01); *A61B 2018/1412* (2013.01); *A61B 2018/1455* (2013.01); *A61B 2018/1861* (2013.01); *A61B 2090/034* (2016.02)

(58) **Field of Classification Search**

CPC .. *A61B 2017/00539*; *A61B 2017/2926*; *A61B 2018/00077*; *A61B 2018/00178*; *A61B 2018/00196*; *A61B 2018/00404*; *A61B 2018/0063*; *A61B 2018/126*; *A61B 2018/1412*; *A61B 2018/1455*; *A61B 2018/1861*; *A61B 2090/034*; *A61B 90/03*
 See application file for complete search history.

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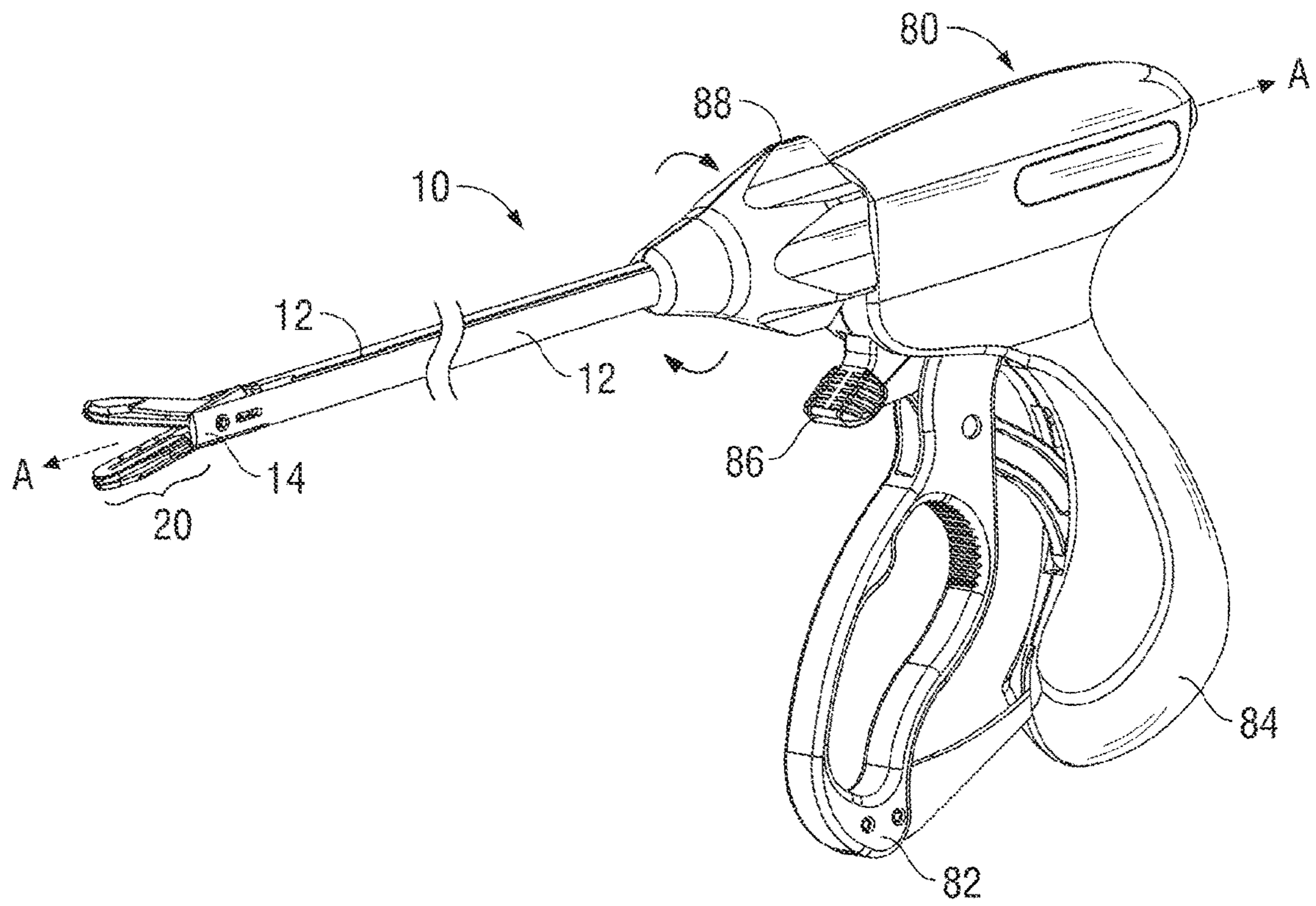


FIG. 1

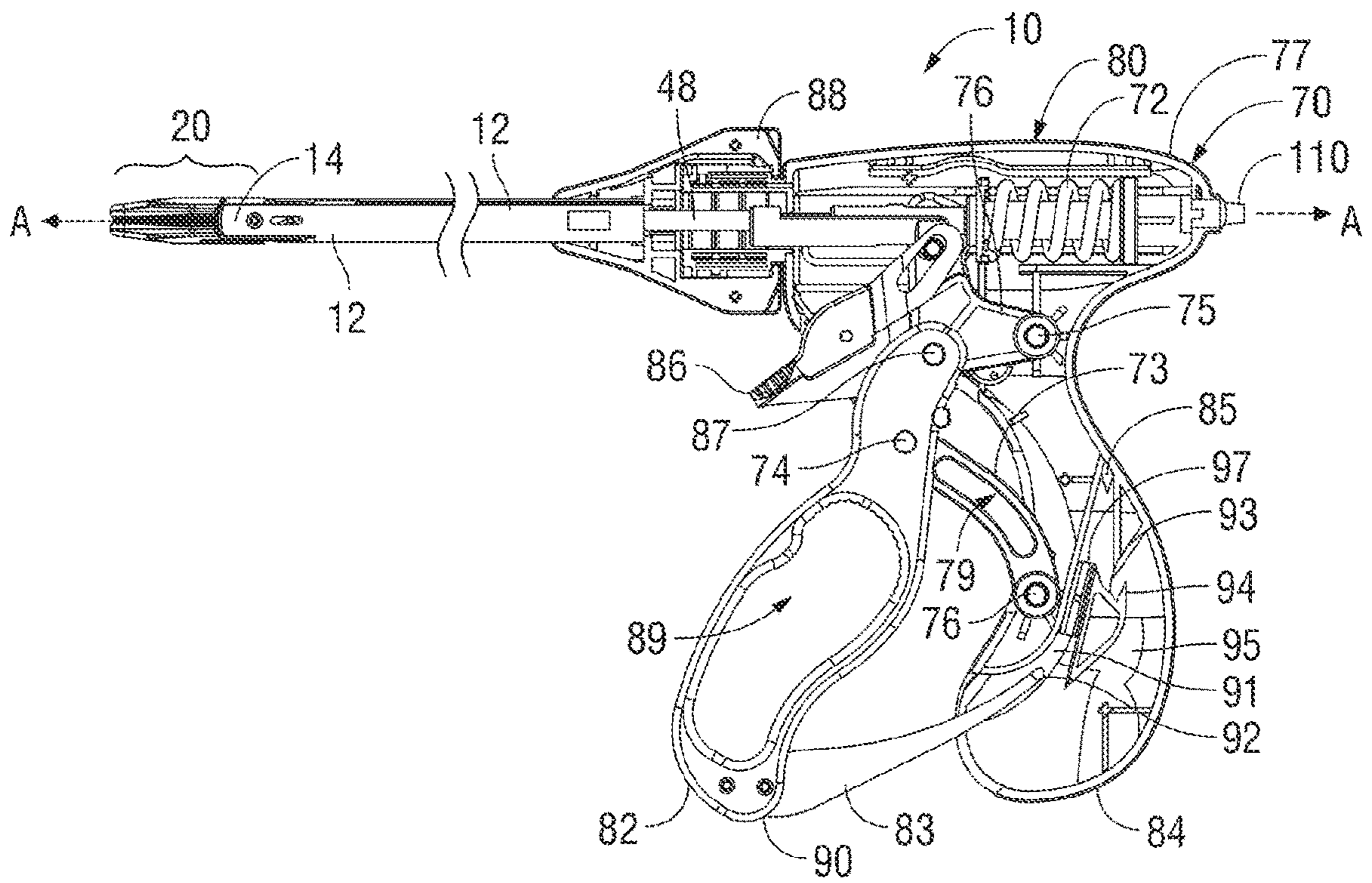


FIG. 2

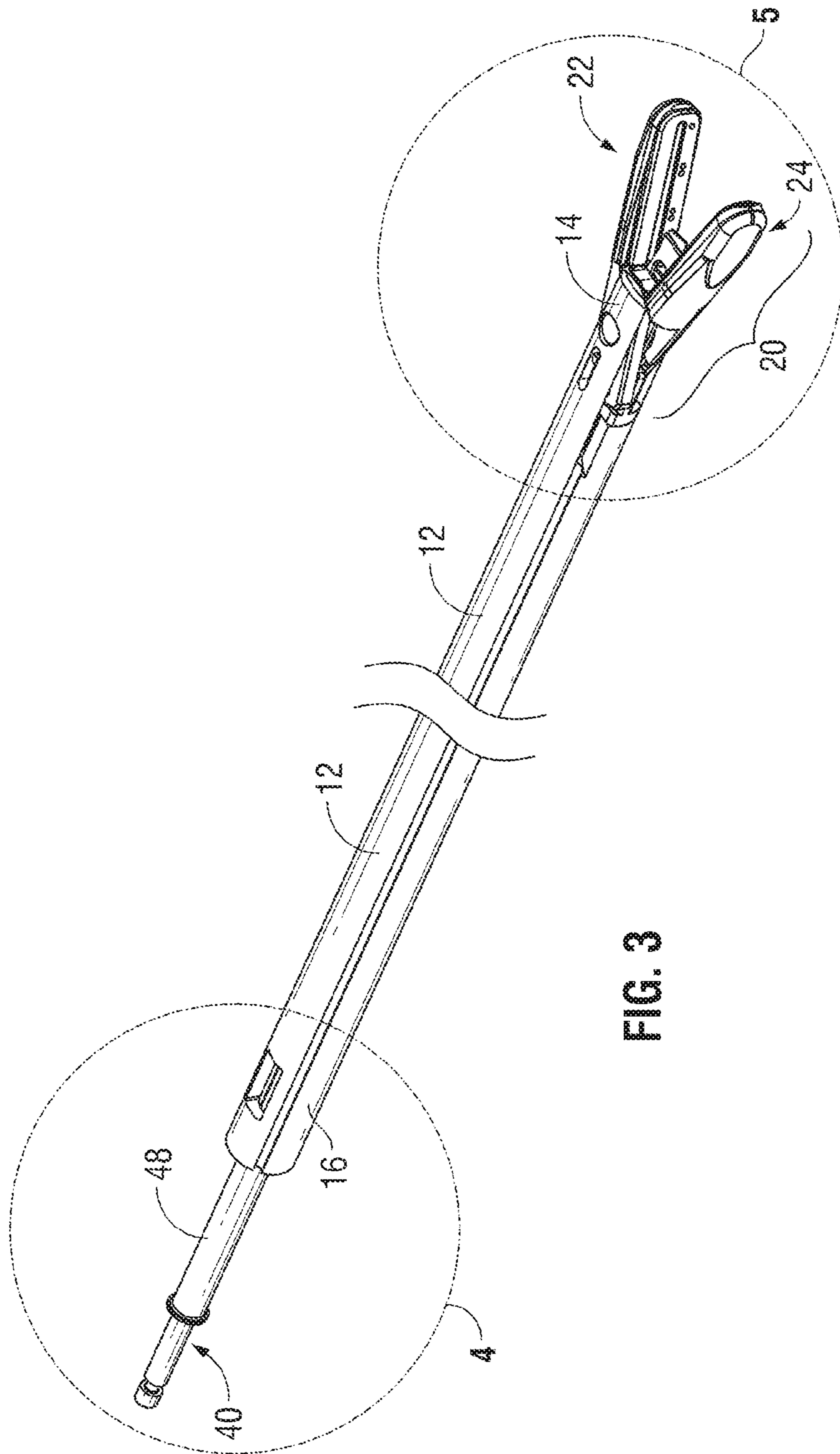


FIG. 3

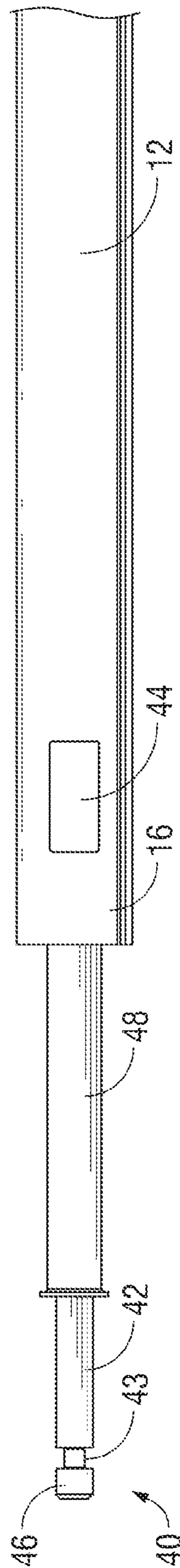


FIG. 4

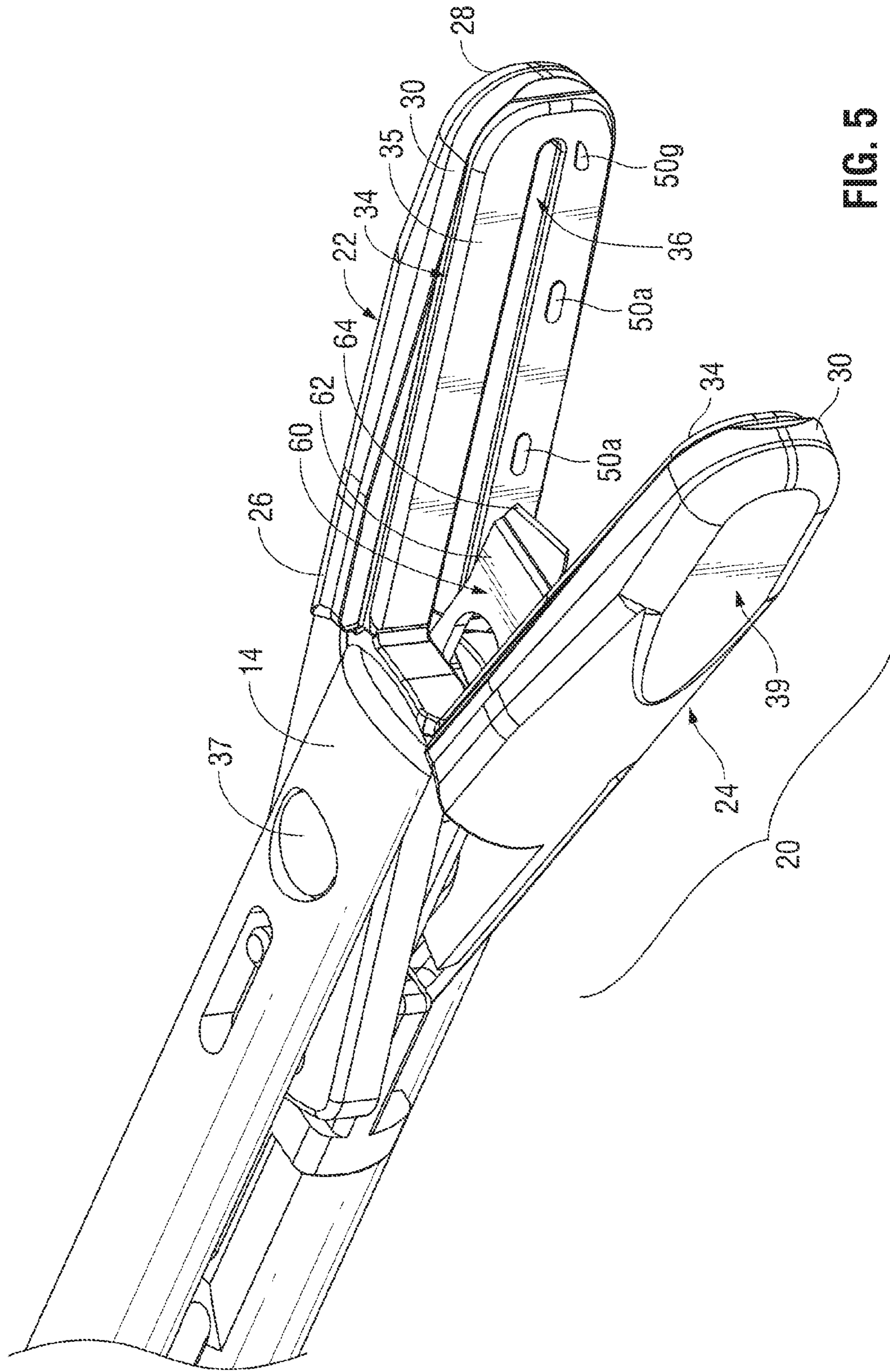


FIG. 5

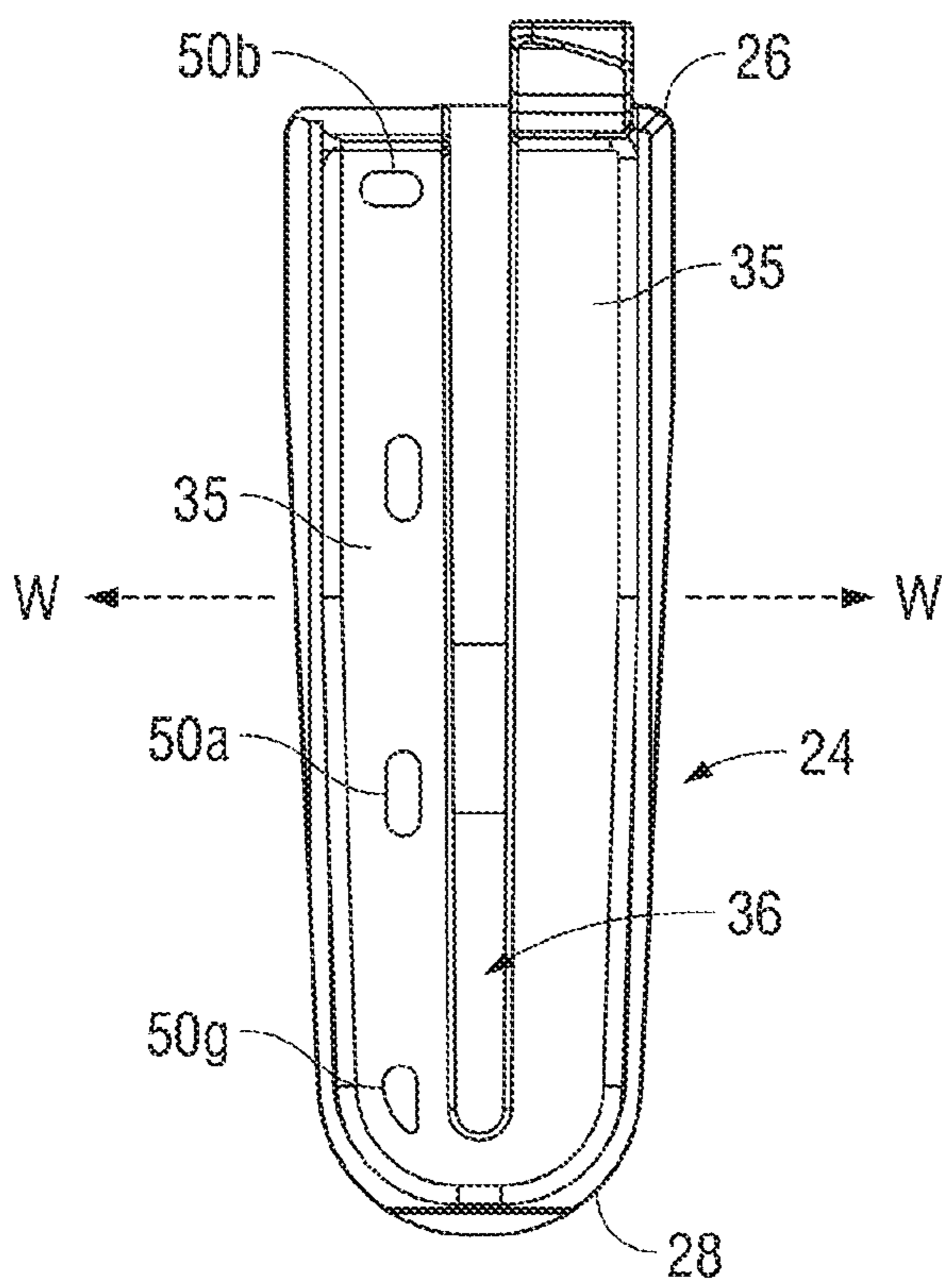


FIG. 6A

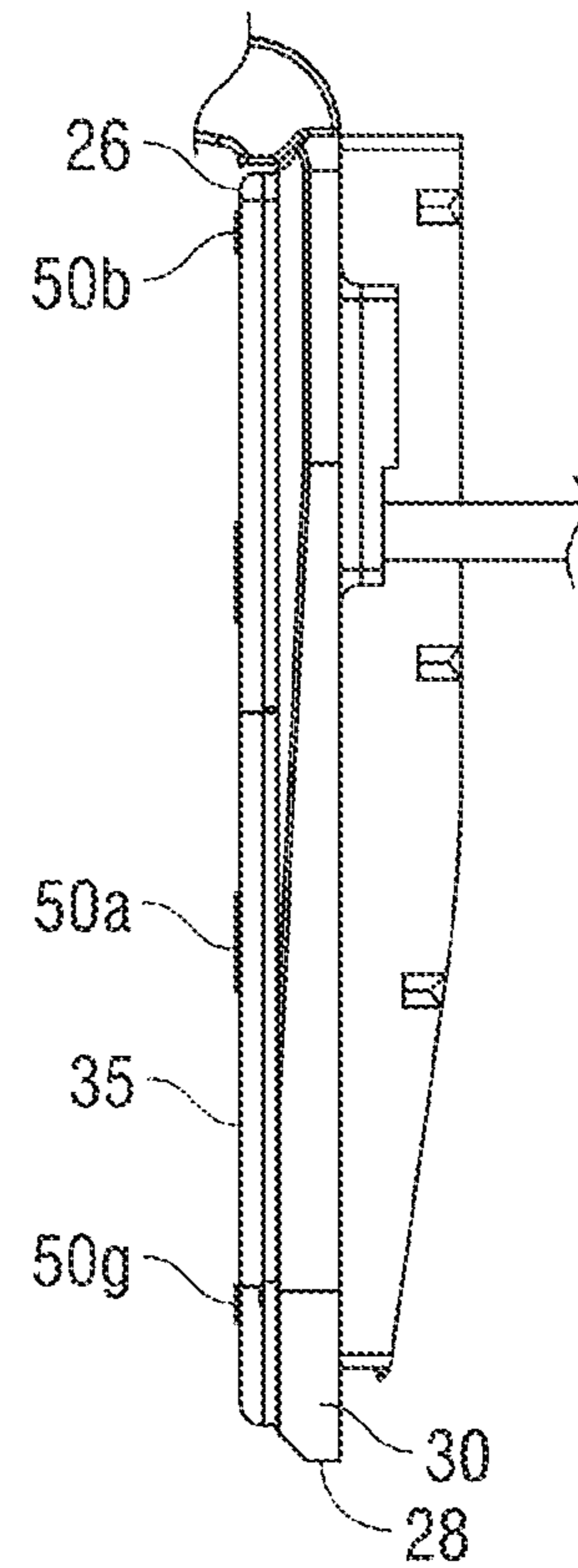


FIG. 6B

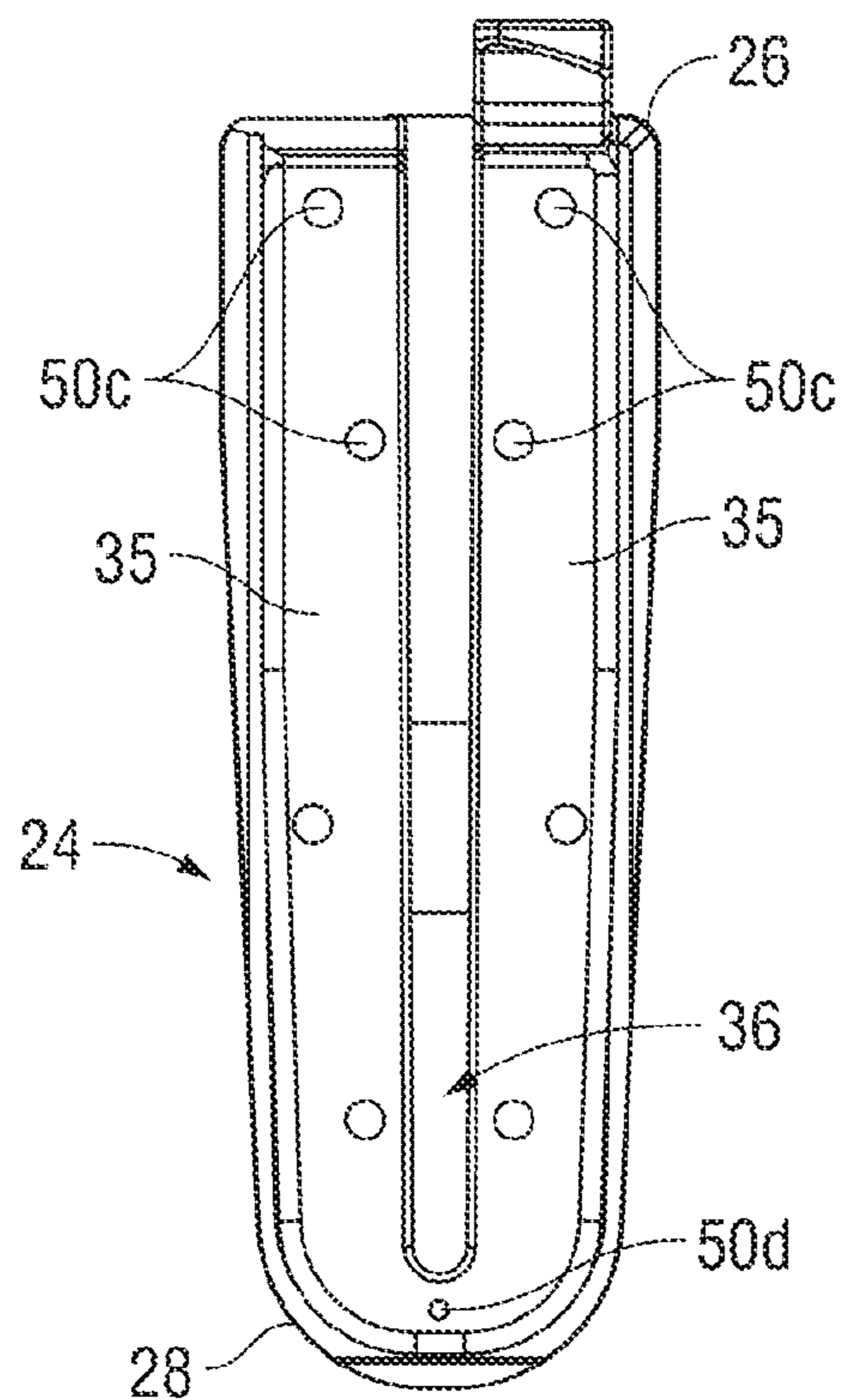


FIG. 6C

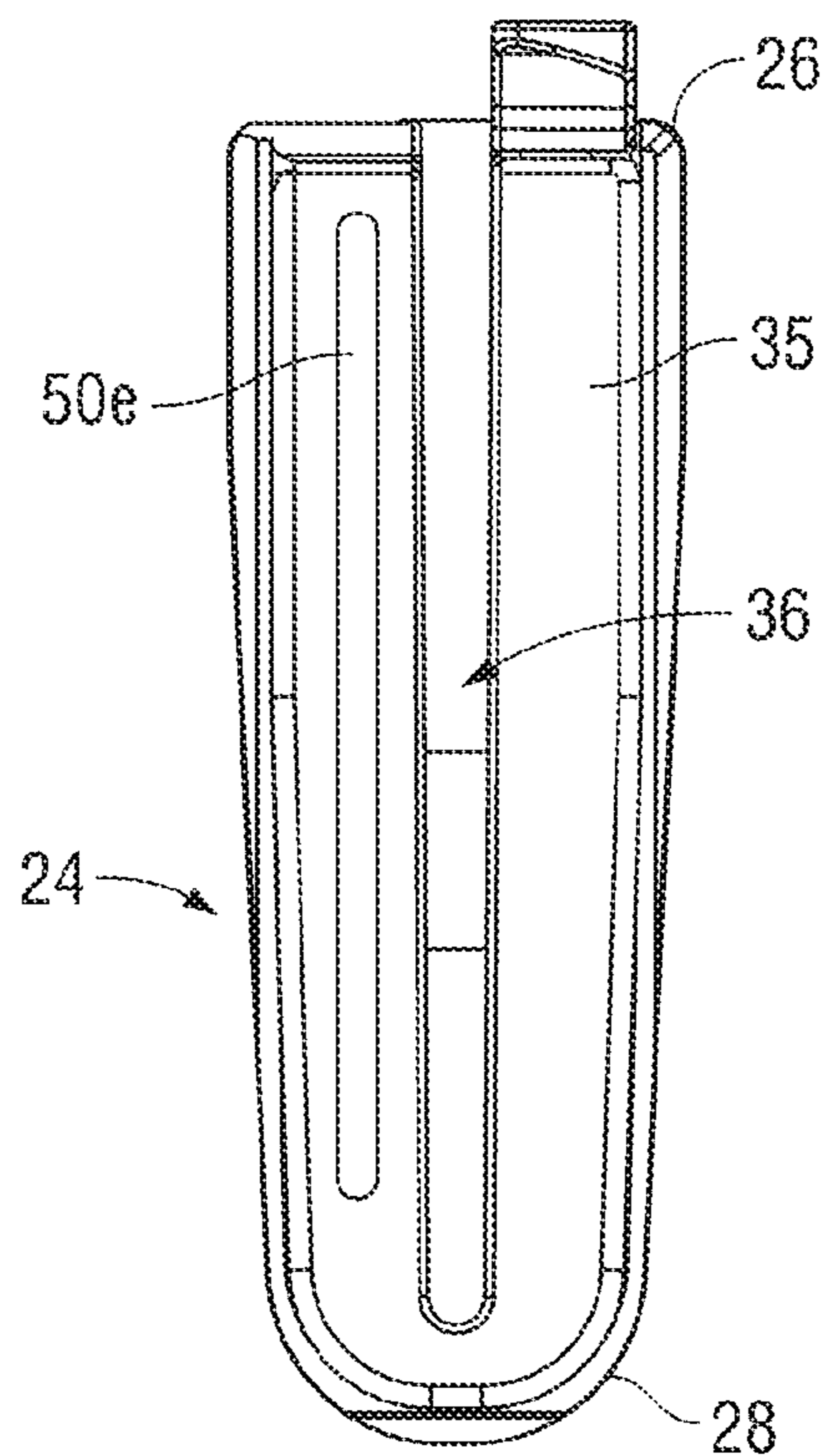


FIG. 6D

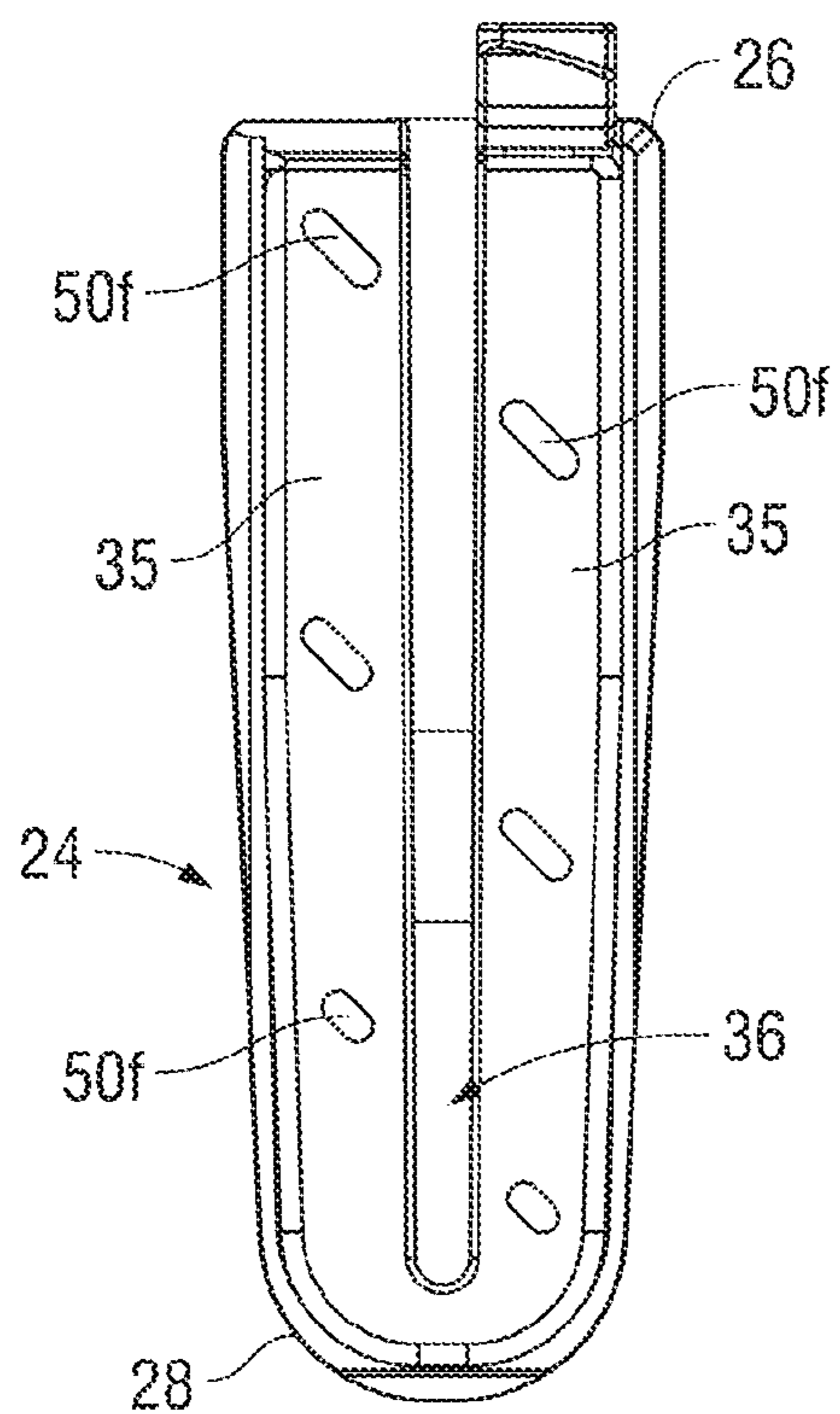


FIG. 6E

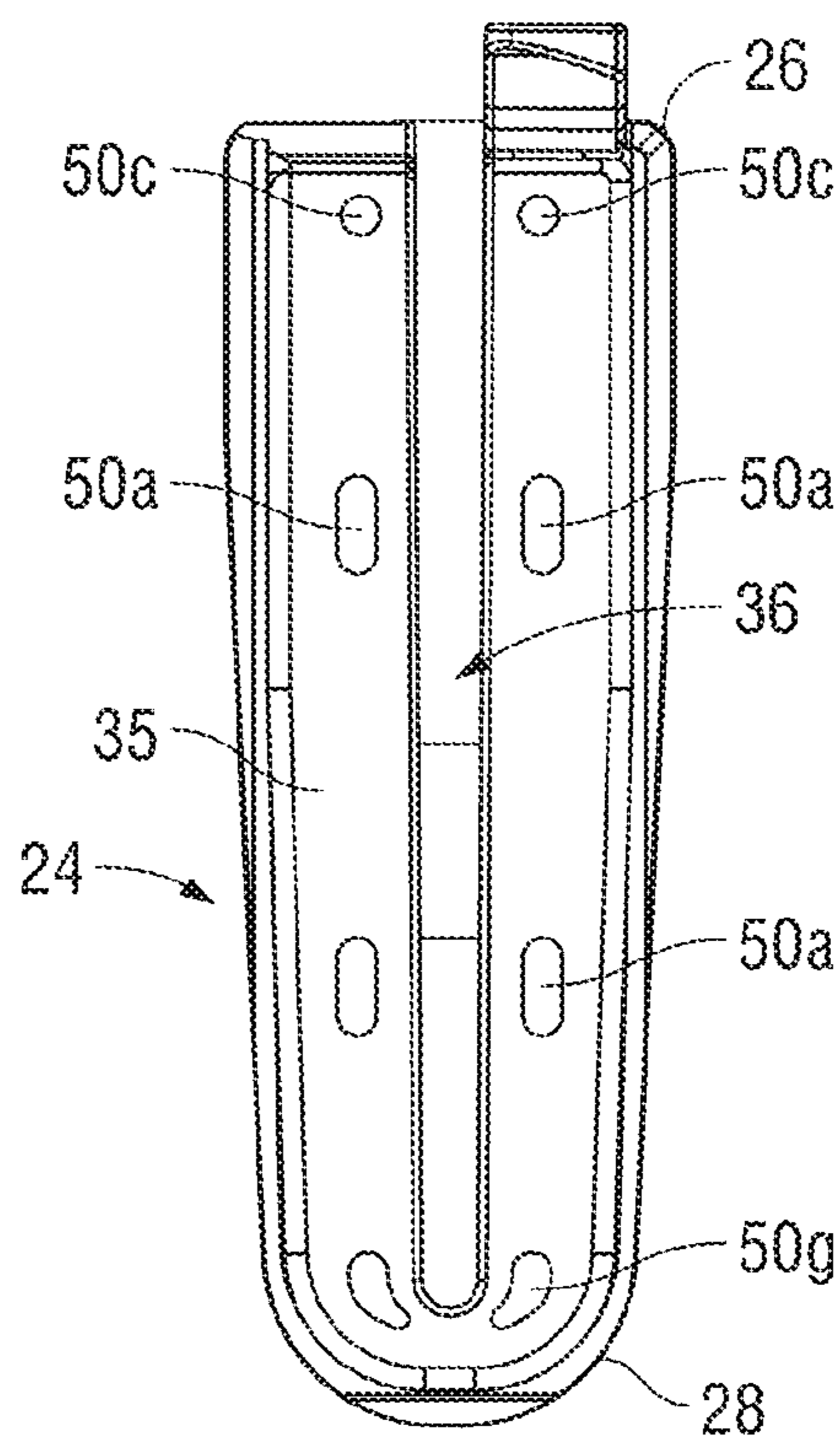


FIG. 6F

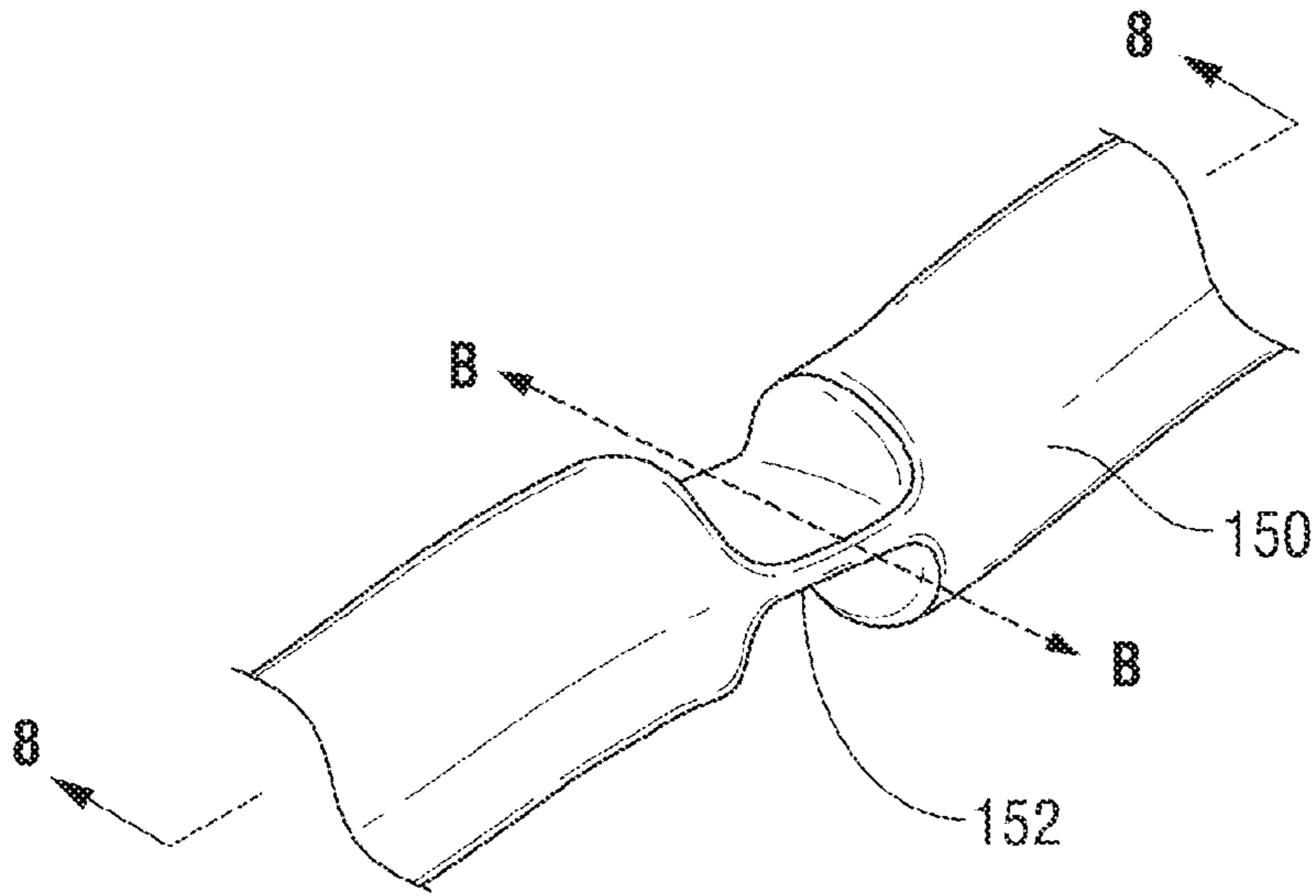


FIG. 7

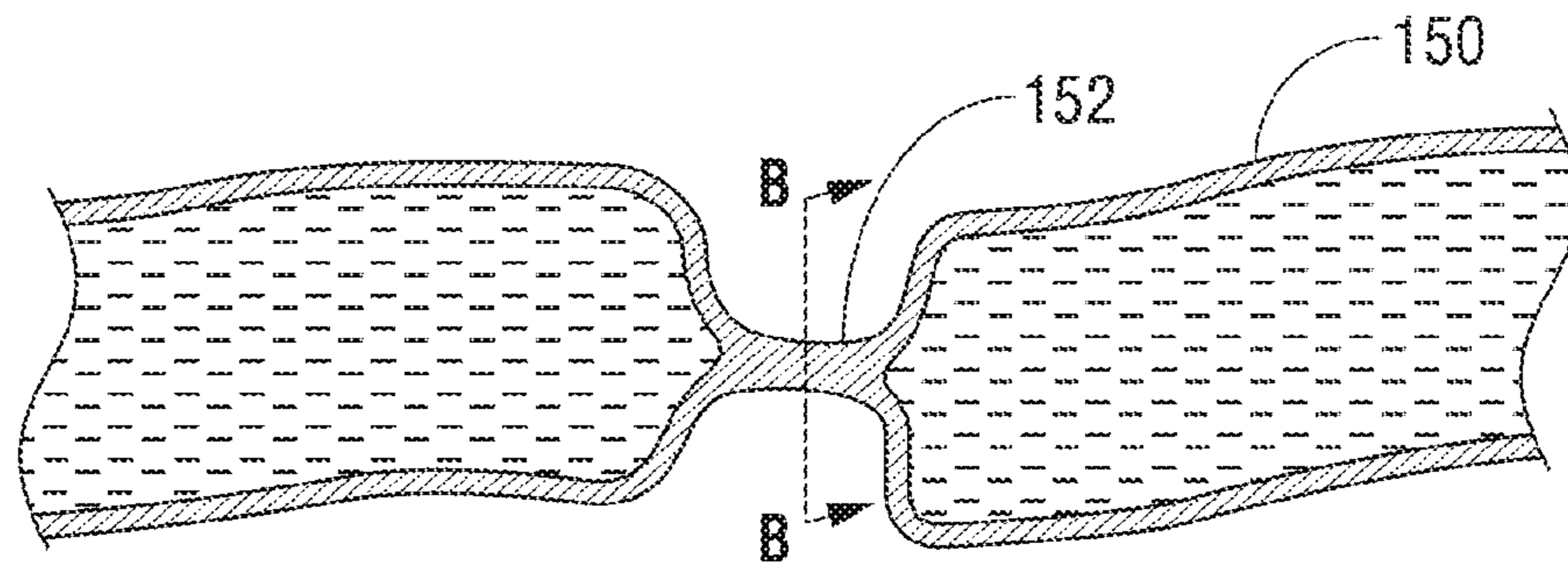


FIG. 8

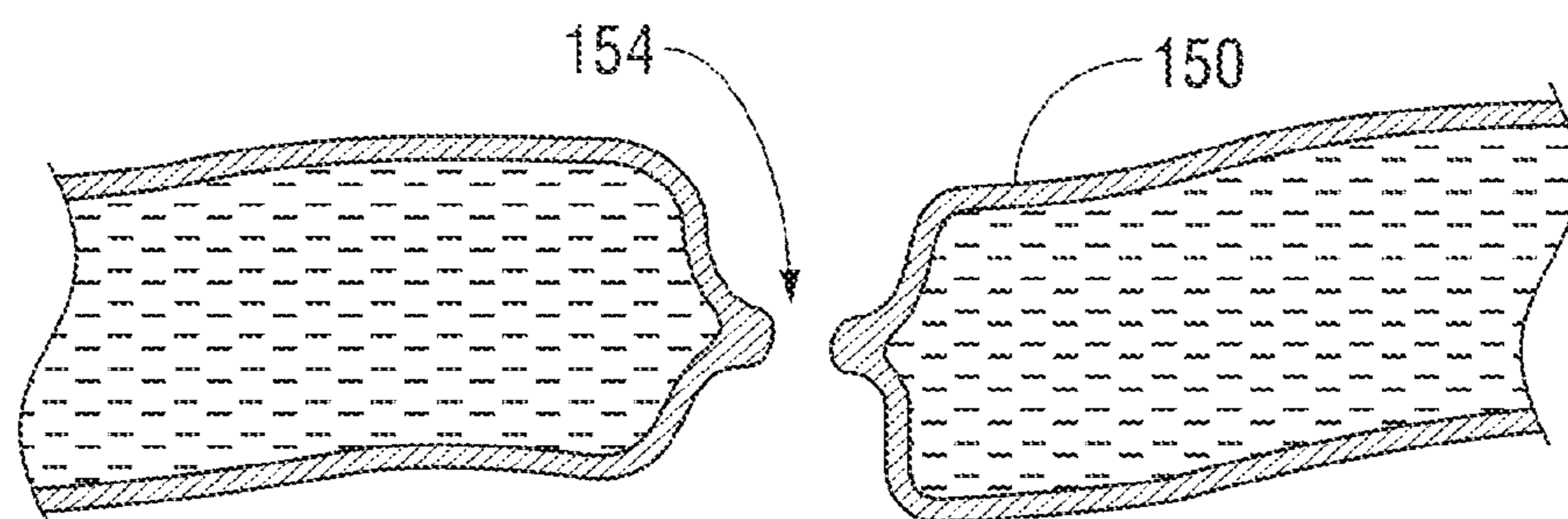


FIG. 9

VESSEL SEALER AND DIVIDER**CROSS-REFERENCE TO RELATED APPLICATIONS**

This application is a continuation of U.S. application Ser. No. 16/053,052, filed on Aug. 2, 2018, now U.S. Pat. No. 10,265,121, which is a continuation of U.S. application Ser. No. 15/911,739, filed on Mar. 5, 2018, now U.S. Pat. No. 10,251,696, which is a continuation of U.S. application Ser. No. 15/338,663, filed on Oct. 31, 2016, which is a continuation of U.S. application Ser. No. 14/719,887, filed on May 22, 2015, which is a continuation of U.S. application Ser. No. 13/584,194, filed on Aug. 13, 2012, which is a continuation of U.S. application Ser. No. 12/348,748, filed on Jan. 5, 2009, now U.S. Pat. No. 8,241,284, which is a continuation of U.S. application Ser. No. 10/471,818, filed on Sep. 11, 2003, now U.S. Pat. No. 7,473,253, which claims the benefit of and priority to PCT Application Serial No. PCT/US01/11413, filed Apr. 6, 2001, entitled "VESSEL SEALER AND DIVIDER WITH NON-CONDUCTIVE STOP MEMBERS", the entire contents of each of these applications is hereby incorporated by reference.

BACKGROUND

The present disclosure relates to an electro-surgical instrument and method for performing endoscopic surgical procedures. More particularly, the present disclosure relates to an endoscopic bipolar electro-surgical forceps and method of using same which includes a non-conductive stop member associated with one or both of the opposing jaw members. The non-conductive stop member is designed to control the gap distance between opposing jaw members and enhance the manipulation and gripping of tissue during the sealing and dividing process.

TECHNICAL FIELD

Endoscopic forceps utilize mechanical action to constrict, grasp, dissect and/or clamp tissue. Endoscopic electro-surgical forceps utilize both mechanical clamping action and electrical energy to effect hemostasis by heating the tissue and blood vessels to coagulate, cauterize and/or seal tissue.

Endoscopic instruments are inserted into the patient through a cannula, or port, that has been made with a trocar or similar such device. Typical sizes for cannulas range from three millimeters to twelve millimeters. Smaller cannulas are usually preferred, and this presents a design challenge to instrument manufacturers who must find ways to make surgical instruments that fit through the cannulas.

Certain endoscopic surgical procedures require cutting blood vessels or vascular tissue. However, due to space limitations surgeons can have difficulty suturing vessels or performing other traditional methods of controlling bleeding, e.g., clamping and/or tying-off transected blood vessels. Blood vessels, in the range below two millimeters in diameter, can often be closed using standard electro-surgical techniques. However, if a larger vessel is severed, it may be necessary for the surgeon to convert the endoscopic procedure into an open-surgical procedure and thereby abandon the benefits of laparoscopy.

Several journal articles have disclosed methods for sealing small blood vessels using electro-surgery. An article entitled Studies on Coagulation and the Development of an Automatic Computerized Bipolar Coagulator, J. Neurosurg., Volume 75, July 1991, describes a bipolar coagulator which

is used to seal small blood vessels. The article states that it is not possible to safely coagulate arteries with a diameter larger than 2 to 2.5 mm. A second article is entitled Automatically Controlled Bipolar Electrocoagulation—"COA-COMP", Neurosurg. Rev. (1984), pp. 187-190, describes a method for terminating electro-surgical power to the vessel so that charring of the vessel walls can be avoided.

As mentioned above, by utilizing an electro-surgical forceps, a surgeon can either cauterize, coagulate/desiccate and/or simply reduce or slow bleeding, by controlling the intensity, frequency and duration of the electro-surgical energy applied through the jaw members to the tissue. The electrode of each jaw member is charged to a different electric potential such that when the jaw members grasp tissue, electrical energy can be selectively transferred through the tissue.

In order to effect a proper seal with larger vessels, two predominant mechanical parameters must be accurately controlled—the pressure applied to the vessel and the gap distance between the electrodes—both of which are affected by the thickness of the sealed vessel. More particularly, accurate application of pressure is important to oppose the walls of the vessel; to reduce the tissue impedance to a low enough value that allows enough electro-surgical energy through the tissue; to overcome the forces of expansion during tissue heating; and to contribute to the end tissue thickness which is an indication of a good seal. It has been determined that a typical fused vessel wall is optimum between 0.001 and 0.005 inches. Below this range, the seal may shred or tear and above this range the lumens may not be properly or effectively sealed.

Electro-surgical methods may be able to seal larger vessels using an appropriate electro-surgical power curve, coupled with an instrument capable of applying a large closure force to the vessel walls. It is thought that the process of coagulating small vessels is fundamentally different than electro-surgical vessel sealing. For the purposes herein, "coagulation" is defined as a process of desiccating tissue wherein the tissue cells are ruptured and dried. Vessel sealing is defined as the process of liquefying the collagen in the tissue so that it reforms into a fused mass. Thus, coagulation of small vessels is sufficient to permanently close them. Larger vessels need to be sealed to assure permanent closure.

U.S. Pat. No. 2,176,479 to Willis, U.S. Pat. Nos. 4,005,714 and 4,031,898 to Hildebrandt, U.S. Pat. Nos. 5,827,274, 5,290,287 and 5,312,433 to Boebel et al., U.S. Pat. Nos. 4,370,980, 4,552,143, 5,026,370 and 5,116,332 to Lottick, U.S. Pat. No. 5,443,463 to Stern et al., U.S. Pat. No. 5,484,436 to Eggers et al. and U.S. Pat. No. 5,951,549 to Richardson et al., all relate to electro-surgical instruments for coagulating, cutting and/or sealing vessels or tissue. However, some of these designs may not provide uniformly reproducible pressure to the blood vessel and may result in an ineffective or non-uniform seal.

For the most part, these instruments rely on clamping pressure alone to procure proper sealing thickness and are not designed to take into account gap tolerances and/or parallelism and flatness requirements which are parameters which, if properly controlled, can assure a consistent and effective tissue seal. For example, it is known that it is difficult to adequately control thickness of the resulting sealed tissue by controlling clamping pressure alone for either of two reasons: 1) if too much force is applied, there is a possibility that the two poles will touch and energy will not be transferred through the tissue resulting in an ineffective seal; or 2) if too low a force is applied the tissue may

pre-maturely move prior to activation and sealing and/or a thicker, less reliable seal may be created.

Typically and particularly with respect to endoscopic electrosurgical procedures, once a vessel is sealed, the surgeon has to remove the sealing instrument from the operative site, substitute a new instrument through the cannula and accurately sever the vessel along the newly formed tissue seal. As can be appreciated, this additional step may be both time consuming (particularly when sealing a significant number of vessels) and may contribute to imprecise separation of the tissue along the sealing line due to the misalignment or misplacement of the severing instrument along the center of the tissue sealing line.

Several attempts have been made to design an instrument which incorporates a knife or blade member which effectively severs the tissue after forming a tissue seal. For example, U.S. Pat. No. 5,674,220 to Fox et al. discloses a transparent vessel sealing instrument which includes a longitudinally reciprocating knife which severs the tissue once sealed. The instrument includes a plurality of openings which enable direct visualization of the tissue during the sealing and severing process. This direct visualization allows a user to visually and manually regulate the closure force and gap distance between jaw members to reduce and/or limit certain undesirable effects known to occur when sealing vessels, thermal spread, charring, etc. As can be appreciated, the overall success of creating a tissue seal with this instrument is greatly reliant upon the user's expertise, vision, dexterity, and experience in judging the appropriate closure force, gap distance and length of reciprocation of the knife to uniformly, consistently and effectively seal the vessel and separate the tissue at the seal.

U.S. Pat. No. 5,702,390 to Austin et al. discloses a vessel sealing instrument which includes a triangularly-shaped electrode which is rotatable from a first position to seal tissue to a second position to cut tissue. Again, the user must rely on direct visualization and expertise to control the various effects of sealing and cutting tissue.

Thus, a need exists to develop an endoscopic electrosurgical instrument which effectively and consistently seals and separates vascular tissue and solves the aforementioned problems. This instrument regulates the gap distances between opposing jaws members, reduces the chances of short circuiting the opposing jaws during activation and assists in manipulating, gripping and holding the tissue prior to and during activation and separation of the tissue.

SUMMARY

The present disclosure relates to an endoscopic bipolar electrosurgical forceps for clamping, sealing and/or dividing tissue. The forceps includes an elongated shaft having opposing jaw members at a distal end thereof. The jaw members are movable relative to one another from a first position wherein the jaw members are disposed in spaced relation relative to one another to a second position wherein the jaw members cooperate to grasp tissue therebetween. An electrosurgical energy source is connected to the jaw members such that the jaw members are capable of conducting energy through tissue held therebetween to effect a tissue seal. At least one non-conductive and spaced-apart stop member is disposed on an inner-facing surface of at least one of the jaw members and is positioned to control the gap distance between the opposing jaw members when the tissue is held therebetween. A longitudinally reciprocating knife severs the tissue proximate the sealing site once an effective seal is formed.

One embodiment of the presently disclosed forceps includes a drive rod assembly which connects the jaw members to the source of electrical energy such that the first jaw member has a first electrical potential and the second jaw member has a second electrical potential. Preferably, a handle mechanically engages the drive rod assembly and imparts movement of the first and second jaw members relative to one another.

In one embodiment of the present disclosure, one of the jaw members includes an electrically conductive surface having a longitudinally-oriented channel defined therein which facilitates longitudinal reciprocation of the knife for severing tissue. Preferably, the forceps includes a trigger for actuating the knife which is independently operable from the drive assembly.

In one embodiment, the forceps includes at least two stop members arranged as a series of longitudinally-oriented projections which extend along the inner-facing surface from the proximal end to the distal end of the jaw member. In another embodiment, the stop members include a series of circle-like tabs which project from the inner facing surface and extend from the proximal end to the distal end of the jaw member. The stop members may be disposed on either opposing jaw member on opposite sides of the longitudinally-oriented channel and/or in an alternating, laterally-offset manner relative to one another along the length of the surface of either or both jaw members.

In another embodiment of the present disclosure, a raised lip is provided to act as a stop member which projects from the inner-facing surface and extends about the outer periphery of the jaw member to control the gap distance between opposing jaw members. In another embodiment, at least one longitudinally-oriented ridge extends from the proximal end to the distal end of one of the jaw members and controls the gap distance between the jaw members.

Preferably, the stop members are affixed/attached to the jaw member(s) by stamping, thermal spraying, overmolding and/or by an adhesive. The stop members project from about 0.001 inches to about 0.005 inches and, preferably, from about 0.002 inches to about 0.003 inches from the inner-facing surface of at least one of the jaw members. It is envisioned that the stop members may be made from an insulative material such as parylene, nylon and/or ceramic. Other materials are also contemplated, e.g., syndiotactic polystyrenes such as QUESTRA® manufactured by DOW Chemical, Syndiotactic-polystyrene (SPS), Polybutylene Terephthalate (PBT), Polycarbonate (PC), Acrylonitrile Butadiene Styrene (ABS), Polyphthalamide (PPA), Polyimide, Polyethylene Terephthalate (PET), Polyamide-imide (PAI), Acrylic (PMMA), Polystyrene (PS and HIPS), Polyether Sulfone (PES), Aliphatic Polyketone, Acetal (POM) Copolymer, Polyurethane (PU and TPU), Nylon with Polyphenylene-oxide dispersion and Acrylonitrile Styrene Acrylate.

Another embodiment of the present disclosure includes an endoscopic bipolar forceps for sealing and dividing tissue having at least one elongated shaft having opposing jaw members at a distal end thereof. The jaw members are movable relative to one another from a first position wherein the jaw members are disposed in spaced relation relative to one another to a second position wherein the jaw members cooperate to grasp tissue therebetween. A drive rod assembly connects the jaw members to a source of electrical energy such that the first jaw member has a first electrical potential and the second jaw member has a second electrical potential. The jaw members, when activated, conduct energy through the tissue held between the jaw members to effect a

tissue seal. A handle attaches to the drive rod assembly and, when actuated, imparts movement of the first and second jaw members relative to one another via the drive rod assembly. At least one non-conductive and spaced-apart stop member is disposed on the inner facing surface of one of the jaw members and operates to control the overall gap distance between the opposing seal surfaces of the jaw members when tissue is held therebetween. A trigger mechanically activates a knife for severing the tissue proximate the tissue sealing site.

The present disclosure also relates to a method for sealing and dividing tissue and includes the steps of providing an endoscopic bipolar forceps which includes an elongated shaft having opposing jaw members at a distal end thereof which cooperate to grasp tissue therebetween, at least one non-conductive and spaced-apart stop member disposed on an inner facing surface of at least one of the jaw members which controls the distance between the jaw members when tissue is held therebetween, and a knife.

The method further includes the steps of: connecting the jaw members to a source of electrical energy; actuating the jaw members to grasp tissue between opposing jaw members; conducting energy to the jaw members to through tissue held therebetween to effect a seal; and actuating the knife to sever tissue proximate the seal.

Preferably, at least one of the jaw members of the providing step includes an electrically conductive surface having a longitudinally-oriented channel defined therein which facilitates actuation of the knife in a longitudinally reciprocating fashion within the channel for severing the tissue.

BRIEF DESCRIPTION OF THE DRAWINGS

Various embodiments of the subject instrument are described herein with reference to the drawings wherein:

FIG. 1 is a perspective view of an endoscopic forceps showing a handle and an end effector according to the present disclosure;

FIG. 2 is a partial cross-section of the forceps of FIG. 1 showing the internal working components of the handle and showing the end effector in a closed configuration;

FIG. 3 is an enlarged, perspective view of the end effector assembly shown in open configuration;

FIG. 4 is a greatly enlarged, side view of a proximal end of the end effector of FIG. 3;

FIG. 5 is a greatly enlarged perspective view of a distal end of the end effector of FIG. 3 showing a knife and a series of stop members disposed along an inner facing surface of a jaw member;

FIGS. 6A-6F show various configurations for the stop members on the inner facing surface of one of the jaw members;

FIG. 7 is an enlarged perspective view of a sealing site of a tubular vessel;

FIG. 8 is a longitudinal cross-section of the sealing site taken along line 8-8 of FIG. 7; and

FIG. 9 is a longitudinal cross-section of the sealing site of FIG. 7 after separation of the tubular vessel.

DETAILED DESCRIPTION

Referring now to FIGS. 1-5, one embodiment of an endoscopic bipolar forceps 10 is shown for use with various surgical procedures and includes a housing and handle assembly 80 having an end effector assembly 20 attached thereto. More particularly, forceps 10 includes a shaft 12 which has a distal end 14 dimensioned to mechanically

engage with the end effector assembly 20 and a proximal end 16 which mechanically engages the housing and handle assembly 80. In the drawings and in the descriptions which follow, the term "proximal", as is traditional, will refer to the end of the forceps 10 which is closer to the user, while the term "distal" will refer to the end which is further from the user.

The end effector assembly 20 is attached to the distal end 14 of shaft 12 and includes a pair of opposing jaw members 22 and 24. Preferably, housing and handle assembly 80 is attached to the proximal end 16 of shaft 12 and includes internally-disposed activating mechanisms, e.g., a movable handle 82 and a drive assembly 70, which mechanically cooperate to impart movement of the jaw members 22 and 24 from an open position wherein the jaw members 22 and 24 are disposed in spaced relation relative to one another, to a clamping or closed position wherein the jaw members 22 and 24 cooperate to grasp tissue 150 (FIG. 7) therebetween.

It is envisioned that the forceps 10 may be designed such that it is fully or partially disposable depending upon a particular purpose or to achieve a particular result. For example, end effector assembly 20 may be selectively and releasably engageable with the distal end 14 of the shaft 12 and/or the proximal end 16 of the shaft 12 may be selectively and releasably engageable with the housing and handle assembly 80. In either of these two instances, the forceps 10 would be considered "partially disposable", i.e., a new or different end effector assembly 20 (or end effector assembly 20 and shaft 12) selectively replaces the old end effector assembly 20 as needed.

FIGS. 1 and 2 show the operating elements and the internal-working components of the housing and handle assembly 80 which for the purposes of the present disclosure are generally described herein. The specific functions and operative relationships of these elements and the various internal-working components are described in more detail in commonly assigned, co-pending application U.S. Serial No. PCT/US01/11340, entitled "VESSEL SEALER AND DIVIDER" by Dycus et al. which is being filed concurrently herewith and which is hereby incorporated by reference herein in its entirety.

As best shown in FIG. 2, housing and handle assembly 80 includes movable handle 82 and a fixed handle 84. The movable handle 82 includes an aperture 89 defined there-through which enables a user to grasp and move the handle 82 relative to the fixed handle 84. Movable handle 82 is selectively moveable about a pivot 87 from a first position relative to fixed handle 84 to a second position in closer proximity to the fixed handle 84 which, as explained below, imparts relative movement of the jaw members 22 and 24 relative to one another.

More particularly, housing and handle assembly 80 houses a drive assembly 70 which cooperates with the movable handle 82 to impart movement of the jaw members 22 and 24 from an open position wherein the jaw members 22 and 24 are disposed in spaced relation relative to one another, to a clamping or closed position wherein the jaw members 22 and 24 cooperate to grasp tissue 150 (FIG. 7) therebetween. The general operating parameters of the drive assembly 70 and the internal-working components of the same are explained in a more generalized fashion below but are explained in specific detail in the above-mentioned commonly assigned, co-pending "VESSEL SEALER AND DIVIDER" application. For the purposes of the present disclosure, the housing and handle assembly 80 can generally be characterized as a four-bar mechanical linkage composed of the following elements: movable handle 82, a link

73, a cam-like link 76 and a base link embodied by fixed pivot points 75 and 76. Movement of the handle 82 activates the four-bar linkage which, in turn, actuates the drive assembly 70 for imparting movement of the opposing jaw members 22 and 24 relative to one another to grasp tissue 150 therebetween. It is envisioned that employing a four-bar mechanical linkage will enable the user to gain a significant mechanical advantage when compressing the jaw members 22 and 24 against the tissue 150 as explained in further detail below with respect to the generally disclosed operating parameters of the drive assembly 70.

Preferably, fixed handle 84 includes a channel 85 defined therein which is dimensioned to receive a flange 83 which extends proximally from movable handle 82. Preferably, flange 83 includes a fixed end 90 which is affixed to movable handle 82 and a free end 92 which is dimensioned for facile reception within channel 85 of handle 84. It is envisioned that flange 83 may be dimensioned to allow a user to selectively, progressively and incrementally move jaw members 22 and 24 relative to one another from the open to closed positions. For example, it is also contemplated that flange 83 may include a ratchet-like interface which lockingly engages the movable handle 82 and, therefore, jaw members 22 and 24 at selective, incremental positions relative to one another depending upon a particular purpose. Other mechanisms may also be employed to control and/or limit the movement of handle 82 relative to handle 84 (and jaw members 22 and 24) such as, e.g., hydraulic, semi-hydraulic and/or gearing systems.

As can be appreciated by the present disclosure and as explained in more detail with respect to the above-mentioned commonly assigned, co-pending "VESSEL SEALER AND DIVIDER" application, channel 85 of fixed handle 84 includes an entrance pathway 91 and an exit pathway 95 for reciprocation of flange 83. As best shown in FIG. 2, as handle 82 moves in a generally pivoting fashion towards fixed handle 84 about pivot 87, link 73 rotates about a guide pin 74 disposed within handle 82. As a result, link 73 rotates proximally about a pivot 76. As can be appreciated, the pivoting path of handle 82 relative to fixed handle 84 biases cam-like link 76 to rotate about pivot 75 in a generally proximal direction. Movement of the cam-like link 76 imparts movement to the drive assembly 70 as explained below.

As best shown in FIG. 2, upon initial movement of handle 82 towards fixed handle 84, the free end 92 of flange 83 moves generally proximally and upwardly along entrance pathway 91 until end 92 passes or mechanically engages a rail member 97 disposed along pathway 91. It is envisioned that rail 97 permits movement of flange 83 proximally until the point where end 92 clears rail 97. Once end 92 clears rail 97, distal movement of the handle 82 and flange 83, i.e., release, is redirected by rail 97 into the exit pathway 95.

More particularly, upon initial release, i.e., a reduction in the closing pressure of handle 82 against handle 84, the handle 82 returns slightly distally towards pathway 91 but is directed towards exit pathway 95. At this point, the release or return pressure between the handles 82 and 84 which is attributable and directly proportional to the release pressure associated with the compression of the drive assembly 70 (explained below) causes the end 92 of flange 83 to settle or lock within a catch basin 93. Handle 82 is now secured in position within handle 84 which, in turn, locks the jaw members 22 and 24 in a closed position against the tissue. The instrument is now positioned for selective application of electro-surgical energy to form the tissue seal 152. Again, the various operating elements and their relevant functions are

explained in more detail with respect to the above-mentioned commonly assigned, co-pending "VESSEL SEALER AND DIVIDER" application.

As best shown in FIG. 2, re-initiation or re-grasping of the handle 82 again moves flange 83 generally proximally along the newly re-directed exit path 95 until end 92 clears a lip 94 disposed along exit pathway 95. Once lip 94 is sufficiently cleared, handle 82 and flange 83 are fully and freely releasable from handle 84 along exit pathway 95 upon the reduction of grasping pressure which, in turn, returns the jaw members 22 and 24 to the open, pre-activated position.

As mentioned above, the housing and handle assembly 80 houses a drive assembly 70 which cooperates with the movable handle 82 to impart relative movement of the jaw members 22 and 24 to grasp the tissue 150. The operation of the drive rod assembly 70 and the various working components of the drive assembly 70 are explained in detail in the above-mentioned commonly assigned, co-pending "VESSEL SEALER AND DIVIDER" application.

Generally and for the purposes of the present disclosure, the drive assembly 70 includes a compression spring 72, a drive rod 40 and a compression sleeve 98 (FIG. 2). As best shown in the enlarged view of FIG. 4, the drive rod 40 is telescopically and internally reciprocable within a knife sleeve 48. Movement of the drive rod 40 relative to the knife sleeve 48 imparts movement to the jaw members 22 and 24. A tab member 46 is disposed at a free end 42 of the drive rod 40 which defines a notch 43 between the tab 46 and end 42. The tab 46 and the notch 43 mechanically cooperate with the compression spring 72 to impart movement of the shaft 40 relative to the knife sleeve 48 which, in turn, opens and closes the jaw members 22 and 24 about the tissue 150.

As explained above, movement of the handle assembly 80 via the four-bar linkage, ultimately causes cam-like link 76 to rotate generally clockwise about pivot 75 (i.e. proximally) which, in turn, compresses spring 72 proximally against a flange 77 disposed within the upper portion of the fixed handle 84. Movement of the spring 72, in turn, moves the drive rod 40 relative to the knife sleeve 48 which moves the opposing jaw members 22 and 24 relative to one another. As can be appreciated, the significant mechanical advantage associated with the four-bar linkage permits facile, consistent and uniform compression of the spring 72 which, in turn, permits facile, consistent and uniform compression of the jaw members 22 and 24 about the tissue 150. Other details and advantages of the four-bar mechanical linkage are more fully discussed with respect to the above-mentioned commonly assigned, co-pending "VESSEL SEALER AND DIVIDER" application.

Once the tissue 150 is grasped between opposing jaw members 22 and 24, electro-surgical energy can be supplied to the jaw members 22 and 24 through an electro-surgical interface 110 disposed within the handle 84. Again these features are explained in more detail with respect to the above-mentioned commonly assigned, co-pending "VESSEL SEALER AND DIVIDER" application.

Forceps 10 also includes a trigger 86 which reciprocates the knife sleeve 48 which, in turn, reciprocates a knife 60 disposed within the end effector assembly 20 as explained below (FIG. 5). Once the a tissue seal 152 is formed (FIG. 7), the user can activate the trigger 86 to separate the tissue 150 as shown in FIG. 9 along the tissue seal 152. As can be appreciated, the reciprocating knife 60 allows the user to quickly separate the tissue 150 immediately after sealing without substituting a cutting instrument through the cannula or trocar port (not shown). It is envisioned that the knife 60 also facilitates a more accurate separation of the vessel

150 along an ideal cutting plane “B-B” associated with the newly formed tissue seal **152** (See FIGS. 7-9). Knife **60** preferably includes a sharpened edge **62** for severing the tissue **150** held between the jaw members **22** and **24** at the tissue sealing site **152** (FIG. 7). It is envisioned that knife **60** may also be coupled to the electrosurgical energy source to facilitate separation of the tissue **150** along the tissue seal **152**.

Preferably and as explained in more detail with respect to the above-mentioned commonly assigned, co-pending “VESSEL SEALER AND DIVIDER” application, handle assembly **80** may also include a lockout mechanism (not shown) which restricts activation of trigger **86** until the jaw members **22** and **24** are closed and/or substantially closed about tissue **150**. For example and as best seen in FIG. 2, exit pathway **95** may be dimensioned such that the trigger **86** is only activatable when flange **83** is disposed in a predetermined or predefined position which provides sufficient clearance for the activation of the trigger **86**, e.g., seated within catch basin **93**. It is envisioned that configuring the handle assembly **80** in this fashion may reduce the chances of premature activation of the trigger **86** prior to electrosurgical activation and sealing.

A rotating assembly **88** may also be incorporated with forceps **10**. Preferably, rotating assembly **88** is mechanically associated with the shaft **12** and the drive assembly **70**. As seen best in FIG. 4, the shaft **12** includes an aperture **44** located therein which mechanically interfaces a corresponding detent (not shown) affixed to rotating assembly **88** such that rotational movement of the rotating assembly **88** imparts similar rotational movement to the shaft **12** which, in turn, rotates the end effector assembly **20** about a longitudinal axis “A”. These features along with the unique electrical configuration for the transference of electrosurgical energy through the handle assembly **80**, the rotating assembly **88** and the drive assembly **70** are described in more detail in the above-mentioned commonly assigned, co-pending “VESSEL SEALER AND DIVIDER” application.

As best seen with respect to FIGS. 3, 5 and 6A-6F, end effector assembly **20** attaches to the distal end **14** of shaft **12**. The end effector assembly **20** includes the first jaw member **22**, the second jaw member **24** and the reciprocating knife **60** disposed therebetween. The jaw members **22** and **24** are preferably pivotable about a pivot **37** from the open to closed positions upon relative reciprocation, i.e., longitudinal movement, of the drive rod **42** as mentioned above. Again, the mechanical and cooperative relationships with respect to the various moving elements of the end effector assembly **20** are further described with respect to the above-mentioned commonly assigned, co-pending “VESSEL SEALER AND DIVIDER” application.

Each of the jaw members includes an electrically conductive sealing surface **35** disposed on inner-facing surface **34** thereof and an insulator **30** disposed on an outer-facing surface **39** thereof. It is envisioned that the electrically conductive surfaces **35** cooperate to seal tissue **150** held therebetween upon the application of electrosurgical energy. The insulators **30** together with the outer, non-conductive surfaces **39** of the jaw members **22** and **24** are preferably dimensioned to limit and/or reduce many of the known undesirable effects related to tissue sealing, e.g., flashover, thermal spread and stray current dissipation.

It is envisioned that the electrically conductive sealing surfaces **35** may also include a pinch trim which facilitates secure engagement of the electrically conductive surface **35** to the insulator **30** and also simplifies the overall manufac-

turing process. It is envisioned that the electrically conductive sealing surface **35** may also include an outer peripheral edge which has a radius and the insulator **30** meets the electrically conductive sealing surface **35** along an adjoining edge which is generally tangential to the radius and/or meets along the radius. Preferably, at the interface, the electrically conductive surface **35** is raised relative to the insulator **30**. These and other envisioned embodiments are discussed in concurrently-filed, co-pending, commonly assigned Application Serial No. PCT/US01/11412 entitled “ELECTROSURGICAL INSTRUMENT WHICH REDUCES COLLATERAL DAMAGE TO ADJACENT TISSUE” by Johnson et al. and concurrently-filed, co-pending, commonly assigned Application Serial No. PCT/US01/11411 entitled “ELECTROSURGICAL INSTRUMENT WHICH IS DESIGNED TO REDUCE THE INCIDENCE OF FLASHOVER” by Johnson et al. The entire contents of both of these applications are hereby incorporated by reference herein.

Preferably, a least one of the electrically conductive surfaces **35** of the jaw members, e.g., **22**, includes a longitudinally-oriented channel **36** defined therein which extends from a proximal end **26** to a distal end **28** of the jaw member **22**. It is envisioned that the channel **36** facilitates longitudinal reciprocation of the knife **60** along a preferred cutting plane “B-B” to effectively and accurately separate the tissue **150** along the formed tissue seal **152** (See FIGS. 7-9). Preferably and as explained in detail in the above-mentioned commonly assigned, co-pending “VESSEL SEALER AND DIVIDER” application, the jaw members **22** and **24** of the end effector assembly **20** are electrically isolated from one another such that electrosurgical energy can be effectively transferred through the tissue **150** to form seal **152**.

As mentioned above, upon movement of the handle **82**, the jaw members **22** and **24** close together and grasp tissue **150**. At this point flange **83** becomes seated within catch **93** which, together with the mechanical advantage associated with the four-bar mechanism and the spring **70**, maintains a proportional axial force on the drive rod **40** which, in turn, maintains a compressive force between opposing jaw members **22** and **24** against the tissue **150**. It is envisioned that the end effector assembly **20** may be dimensioned to off-load excessive clamping forces to prevent mechanical failure of certain internal operating elements of the end effector.

By controlling the intensity, frequency and duration of the electrosurgical energy applied to the tissue **150**, the user can either cauterize, coagulate/desiccate seal and/or simply reduce or slow bleeding. As mentioned above, two mechanical factors play an important role in determining the resulting thickness of the sealed tissue and effectiveness of the seal, i.e., the pressure applied between opposing jaw members **22** and **24** and the gap distance between the opposing sealing surfaces **35** of the jaw members **22** and **24** during the sealing process. However, thickness of the resulting tissue seal **152** cannot be adequately controlled by force alone. In other words, too much force and the two jaw members **22** and **24** would touch and possibly short resulting in little energy traveling through the tissue **150** thus resulting in a bad tissue seal **152**. Too little force and the seal **152** would be too thick.

Applying the correct force is also important for other reasons: to oppose the walls of the vessel; to reduce the tissue impedance to a low enough value that allows enough current through the tissue **150**; and to overcome the forces of expansion during tissue heating in addition to contributing towards creating the required end tissue thickness which is an indication of a good seal.

Preferably, the electrically conductive sealing surfaces 35 of the jaw members 22 and 24 are relatively flat to avoid current concentrations at sharp edges and to avoid arcing between high points. In addition and due to the reaction force of the tissue 150 when engaged, jaw members 22 and 24 are preferably manufactured to resist bending. For example and as best seen in FIG. 6A, the jaw members 22 and 24 are preferably tapered along width "W" which is advantageous for two reasons: 1) the taper will apply constant pressure for a constant tissue thickness at parallel; 2) the thicker proximal portion of the jaw members 22 and 24 will resist bending due to the reaction force of the tissue 150.

As best seen in FIGS. 5-6F, in order to achieve a desired spacing between the electrically conductive surfaces 35 of the respective jaw members 22 and 24, (i.e., gap distance) and apply a desired force to seal the tissue 150, at least one jaw member 22 and/or 24 includes at least one stop member, e.g., 50a, which limits the movement of the two opposing jaw members 22 and 24 relative to one another. Preferably, the stop member, e.g., 50a, extends from the sealing surface or tissue contacting surface 35 a predetermined distance according to the specific material properties (e.g., compressive strength, thermal expansion, etc.) to yield a consistent and accurate gap distance during sealing. Preferably, the gap distance between opposing sealing surfaces 35 during sealing ranges from about 0.001 inches to about 0.005 inches and, more preferably, between about 0.002 and about 0.003 inches.

Preferably, stop members 50a-50g are made from an insulative material, e.g., parylene, nylon and/or ceramic and are dimensioned to limit opposing movement of the jaw members 22 and 24 to within the above mentioned gap range. It is envisioned that the stop members 50a-50g may be disposed on one or both of the jaw members 22 and 24 depending upon a particular purpose or to achieve a particular result.

FIGS. 6A-6F show various contemplated configurations of the non-conductive stop members 50a-50g disposed on, along or protruding through the jaw member 24. It is envisioned that one or more stop members, e.g., 50a and 50g, can be positioned on either or both jaw members 22 and 24 depending upon a particular purpose or to achieve a desired result. As can be appreciated by the present disclosure, the various configurations of the stop members 50a-50g are designed to both limit the movement of the tissue 150 prior to and during activation and prevent short circuiting of the jaw members 22 and 24 as the tissue 150 is being compressed.

FIGS. 6A and 6B show one possible configuration of the stop members 50a-50g for controlling the gap distance between opposing seal surfaces 35. More particularly, a pair of longitudinally-oriented tab-like stop members 50a are disposed proximate the center of sealing surface 35 on one side of the knife channel 36 of jaw member 24. A second stop member, e.g., 50b, is disposed at the proximal end 26 of jaw member 24 and a third stop member 50g is disposed at the distal tip 28 of jaw member 24. Preferably, the stop members 50a-50g may be configured in any known geometric or polynomial configuration, e.g., triangular, rectangular, circular, ovoid, scalloped, etc., depending upon a particular purpose. Moreover, it is contemplated that any combination of different stop members 50a-50g may be assembled along the sealing surfaces 35 to achieve a desired gap distance. It is also envisioned that the stop members may be designed as a raised lip (not shown) which projects from the outer periphery of the jaw member 24.

FIG. 6C shows a first series of circle-like stop members 50c extending from the proximal end 26 to the distal end 28 of jaw member 24 in an alternating, laterally-offset manner relative to one another on one side of the knife channel 36 and a second series of circle-like stop members 50c extending from the proximal end 26 to the distal end 28 of jaw member 24 in an alternating, laterally-offset manner relative to one another on the other side of the knife channel 36. It is envisioned that circle-like stop members 50c are substantially equal in size, however, one or more of the stop members 50c may be dimensioned larger or smaller than the other stop members 50c depending upon a particular purpose or to achieve a desired result.

FIG. 6D shows yet another configuration wherein the stop member is configured as a longitudinally-oriented ridge 50e extending from a proximal end 26 to a distal end 28 of jaw member 24 along one side of knife channel 36. As mentioned above, a second longitudinally-oriented ridge 50e may be disposed on opposing jaw member 22 on the opposite side of knife channel 36 for sealing purposes. FIG. 6E shows a series of elongated tab-like members 50f which are disposed at an angle relative to knife channel 36. FIG. 6F shows yet another configuration wherein different stop members, e.g., 50a, 50c and 50g are disposed atop sealing surface 35 on both sides of the knife channel 36.

Preferably, the non-conductive stop members 50a-50g are molded onto the jaw members 22 and 24 (e.g., overmolding, injection molding, etc.), stamped onto the jaw members 22 and 24 or deposited (e.g., deposition) onto the jaw members 22 and 24. The stop members 50a-50g may also be slideably attached to the jaw members and/or attached to the electrically conductive surfaces 35 in a snap-fit manner. Other techniques involve thermally spraying a ceramic material onto the surface of the jaw member 22 and 24 to form the stop members 50a-50g. Several thermal spraying techniques are contemplated which involve depositing a broad range of heat resistant and insulative materials on the electrically conductive surfaces 35 to create stop members 50a-50g, e.g., High velocity Oxy-fuel deposition, plasma deposition, etc.

It is envisioned that the stop members 50a-50g protrude about 0.001 to about 0.005 inches from the inner-facing surfaces 35 of the jaw members 22 and 24 which, as can be appreciated by the present disclosure, both reduces the possibility of short circuiting between electrically conductive surfaces and enhances the gripping characteristics of the jaw members 22 and 24 during sealing and dividing. Preferably, the stop members 50a-50g protrude about 0.002 inches to about 0.003 inches from the electrically conductive surface 35 which has been determined yield an ideal gap distance for producing effective, uniform and consistent tissue seals.

Alternatively, the stop members 50a-50g can be molded onto the inner-facing surface 35 of one or both jaw members 22 and 24 or, in some cases, it may be preferable to adhere the stop member 50a-50g to the inner facing surfaces 35 of one or both of the jaw members 22 and 24 by any known method of adhesion. Stamping is defined herein to encompass virtually any press operation known in the trade, including but not limited to: blanking, shearing, hot or cold forming, drawing, bending, and coining.

FIGS. 6A-6F show some of the possible configurations of the stop members 50a-50f, however, these configurations are shown by way of example and should not be construed as limiting. Other stop member configurations are also contemplated which may be equally effective in reduc-

ing the possibility of short circuiting between electrically conductive surfaces **35** and enhancing tissue grip during sealing and dividing.

Further, although it is preferable that the stop members **50a-50g** protrude about 0.001 inches to about 0.005 and preferably about 0.002 inches to about 0.003 inches from the inner-facing surfaces **35** of the jaw member **22** and **24**, in some cases it may be preferable to have the stop members **50a-50g** protrude more or less depending upon a particular purpose. For example, it is contemplated that the type of material used for the stop members **50a-50g** and that material's ability to absorb the large compressive closure forces between jaw members **22** and **24** will vary and, therefore, the overall dimensions of the stop members **50a-50g** may vary as well to produce the desired gap distance.

In other words, the compressive strength of the material along with the desired or ultimate gap distance required for effective sealing are parameters which are carefully considered when forming the stop members **50a-50g** and one material may have to be dimensioned differently from another material to achieve the same gap distance or desired result. For example, the compressive strength of nylon is different from ceramic and, therefore, the nylon material may have to be dimensioned differently, e.g., thicker, to counteract the closing force of the opposing jaw members **22** and **24** and to achieve the same desired gap distance when utilizing a ceramic stop member.

The present disclosure also relates to a method of sealing and dividing tissue and includes the steps of providing an endoscopic bipolar forceps **10** which includes an elongated shaft **12** having opposing jaw members **22** and **24** at a distal end **14** thereof which cooperate to grasp tissue **150** therebetween, at least one non-conductive and spaced-apart stop member **50a-50g** disposed on an inner facing surface **35** of at least one of the jaw members, e.g., **24**, which controls the distance between the jaw members **22** and **24** when tissue **150** is held therebetween, and a knife **60**.

The method further includes the steps of: connecting the jaw members **22** and **24** to a source **110** of electrical energy; actuating the jaw members **22** and **24** to grasp tissue **150** between opposing jaw members **22** and **24**; conducting energy to the jaw members **22** and **24** to through tissue **150** held therebetween to effect a seal **152** (FIGS. 7-9); and actuating the knife **60** to sever tissue proximate the seal **152**.

Preferably, at least one of the jaw members, e.g., **24**, of the providing step includes an electrically conductive surface **35** having a longitudinally-oriented channel **36** defined therein which facilitates actuation of the knife **60** in a longitudinally reciprocating fashion within the channel **36** for severing the tissue **150** proximate the tissue site.

From the foregoing and with reference to the various figure drawings, those skilled in the art will appreciate that certain modifications can also be made to the present disclosure without departing from the scope of the present disclosure. For example, it may be preferable to add other features to the forceps **10**, e.g., an articulating assembly to axially displace the end effector assembly **20** relative to the elongated shaft **12**.

Moreover, it is contemplated that the presently disclosed forceps may include a disposable end effector assembly which is selectively engageable with at least one portion of the electro-surgical instrument, e.g., shaft **12** and/or handle assembly **80**.

While several embodiments of the disclosure have been shown in the drawings, it is not intended that the disclosure be limited thereto, as it is intended that the disclosure be as broad in scope as the art will allow and that the specification

be read likewise. Therefore, the above description should not be construed as limiting, but merely as exemplifications of a preferred embodiments. Those skilled in the art will envision other modifications within the scope and spirit of the claims appended hereto.

What is claimed is:

1. A bipolar electro-surgical instrument, comprising:

a housing;

a shaft extending distally from the housing;

first and second jaw members disposed at a distal end of the shaft, the first and second jaw members including first and second seal surfaces, respectively, the first and second seal surfaces defining first and second knife channels, respectively, at least one of the first or second jaw members movable relative to the other from an open position to a closed position to grasp tissue between the first and second seal surfaces, the first and second seal surfaces adaptable to connect to a source of electrical energy such that the first and second seal surfaces are capable of conducting energy through tissue grasped therebetween;

a drive rod extending from the housing and through the shaft, the drive rod operably coupled with at least one of the first or second jaw members such that proximal translation of the drive rod moves the at least one of the first or second jaw members relative to the other to the closed position;

a drive linkage including at least a first end portion and a second end portion;

a movable handle coupled to the housing and movable proximally relative to a fixed handle portion of the housing from a spaced-apart position to an approximated position, the movable handle pivotably connected to the first end portion of the drive linkage;

a spring disposed within the housing, wherein a first end portion of the spring is operably coupled to the second end portion of drive linkage and wherein a second end portion of the spring is operably coupled to the drive rod, wherein movement of the drive linkage, in response to proximal movement of the movable handle from the spaced-apart position towards the approximated position moves the spring proximally to translate the drive rod proximally to thereby move the at least one of the first or second jaw members relative to the other to the closed position to maintain a compressive force between the first and second jaw members about tissue grasped between the first and second seal surfaces;

at least one stop member disposed on at least one of the first or second jaw members, the at least one stop member configured to regulate a gap distance between the first and second sealing surfaces in the closed position, wherein the gap distance and the compressive force facilitate sealing tissue grasped between the first and second sealing surfaces; and

a knife configured to translate through the first and second knife channels to cut sealed tissue.

2. The bipolar electro-surgical instrument according to claim 1, wherein the movable handle is configured to move the drive linkage to rotate and wherein rotation of the drive link moves the spring.

3. The bipolar electro-surgical instrument according to claim 1, further comprising a ratchet associated with the fixed handle portion of the housing and the movable handle, the ratchet including flange and a channel, the flange configured to engage the channel upon actuation of the movable handle to lock the movable handle relative to the fixed

15

handle portion of the housing, thereby locking the first and second jaw members in the closed position.

4. The bipolar electrosurgical instrument according to claim 1, further comprising a trigger pivotably coupled to the housing and operably coupled to the knife, wherein actuation of the trigger moves translates the knife through the first and second knife channels.

5. The bipolar electrosurgical instrument according to claim 4, further comprising a knife sleeve extending from the housing and through the shaft, the knife sleeve operably coupling the trigger with the knife, wherein actuation of the trigger translates the knife sleeve to thereby translate the knife through the first and second knife channels.

6. The bipolar electrosurgical instrument according to claim 1, wherein the first and second seal surfaces are disposed on inwardly-facing surfaces of the first and second jaw members, respectively, and wherein each of the first and second jaw members further includes an insulator disposed on an outwardly-facing surface thereof.

7. The bipolar electrosurgical instrument according to claim 1, wherein the at least one stop member includes a plurality of stop members.

16

8. The bipolar electrosurgical instrument according to claim 1, further comprising a tab extending from the drive rod, wherein movement of the spring urges the spring into the tab to translate the drive rod to thereby move the at least one of the first or second jaw members relative to the other to the closed position.

9. The bipolar electrosurgical instrument according to claim 8, wherein the spring is compressed against the tab to translate the drive rod.

10. The bipolar electrosurgical instrument according to claim 1, wherein the spring is disposed about the drive rod.

11. The bipolar electrosurgical instrument according to claim 10, wherein the spring is a compression coil spring.

12. The bipolar electrosurgical instrument according to claim 10, wherein the spring and the drive rod are aligned on a longitudinal axis extending through the shaft.

13. The bipolar electrosurgical instrument according to claim 1, wherein both of the first and second jaw members are movable from the open position to the closed position.

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