



US010681794B1

(12) **United States Patent**
Steck et al.

(10) **Patent No.:** **US 10,681,794 B1**
(45) **Date of Patent:** ***Jun. 9, 2020**

(54) **TRI-AXIS X-RAY TUBE**

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

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This patent is subject to a terminal disclaimer.

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(21) Appl. No.: **16/749,738**

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(22) Filed: **Jan. 22, 2020**

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Related U.S. Application Data

(63) Continuation of application No. 16/144,113, filed on Sep. 27, 2018, now Pat. No. 10,624,195.

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(60) Provisional application No. 62/577,276, filed on Oct. 26, 2017.

(51) **Int. Cl.**

H01J 35/18 (2006.01)

H05G 1/02 (2006.01)

H01J 35/06 (2006.01)

H01J 35/08 (2006.01)

H05G 1/10 (2006.01)

(52) **U.S. Cl.**

CPC **H05G 1/02** (2013.01); **H01J 35/06** (2013.01); **H01J 35/08** (2013.01); **H01J 35/18** (2013.01); **H05G 1/10** (2013.01)

(58) **Field of Classification Search**

None

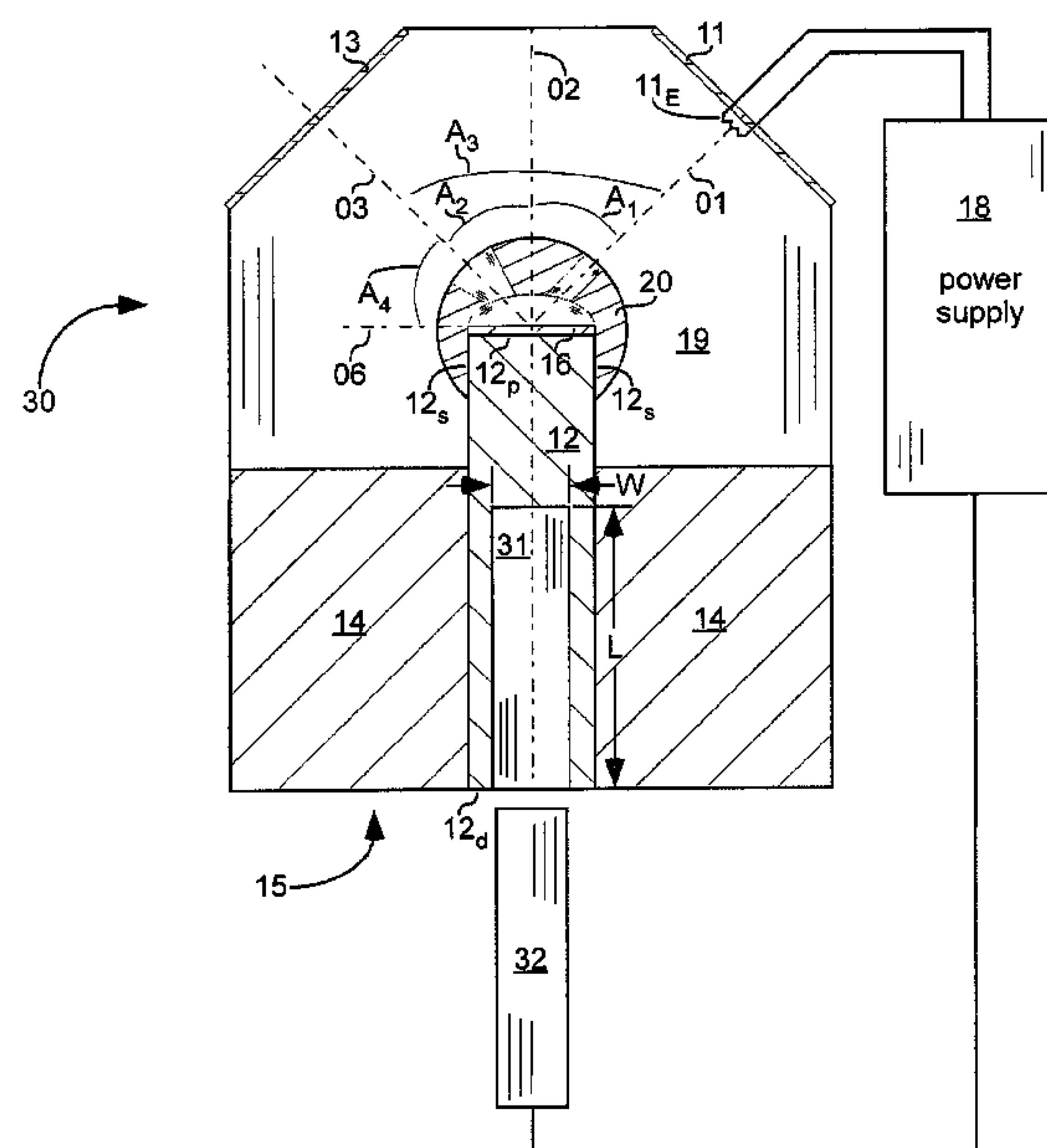
See application file for complete search history.

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ABSTRACT

In one embodiment, an x-ray tube **15** can be used closer to a sample. An angle A_1 between an anode axis **02** and an electron-beam axis **01** can be $\geq 10^\circ$ and $\leq 80^\circ$ and an angle A_2 between the anode axis **02** and an x-ray axis **03** can be $\geq 10^\circ$ and $\leq 80^\circ$. In another embodiment, a cap **20** on an anode **12** can block x-rays emitted in undesired directions. The cap **20** can include an internal cavity **24**, an electron-beam hole **21**, an anode hole **22**, and an x-ray hole **23**. In another embodiment, an electrical connection between an x-ray tube **15** and a power supply **18** can be reliable and easy to manufacture. The anode **12** can include a hole **31** at an end of the anode **12** sized and shaped for insertion of an electrical connector **32**.

20 Claims, 5 Drawing Sheets



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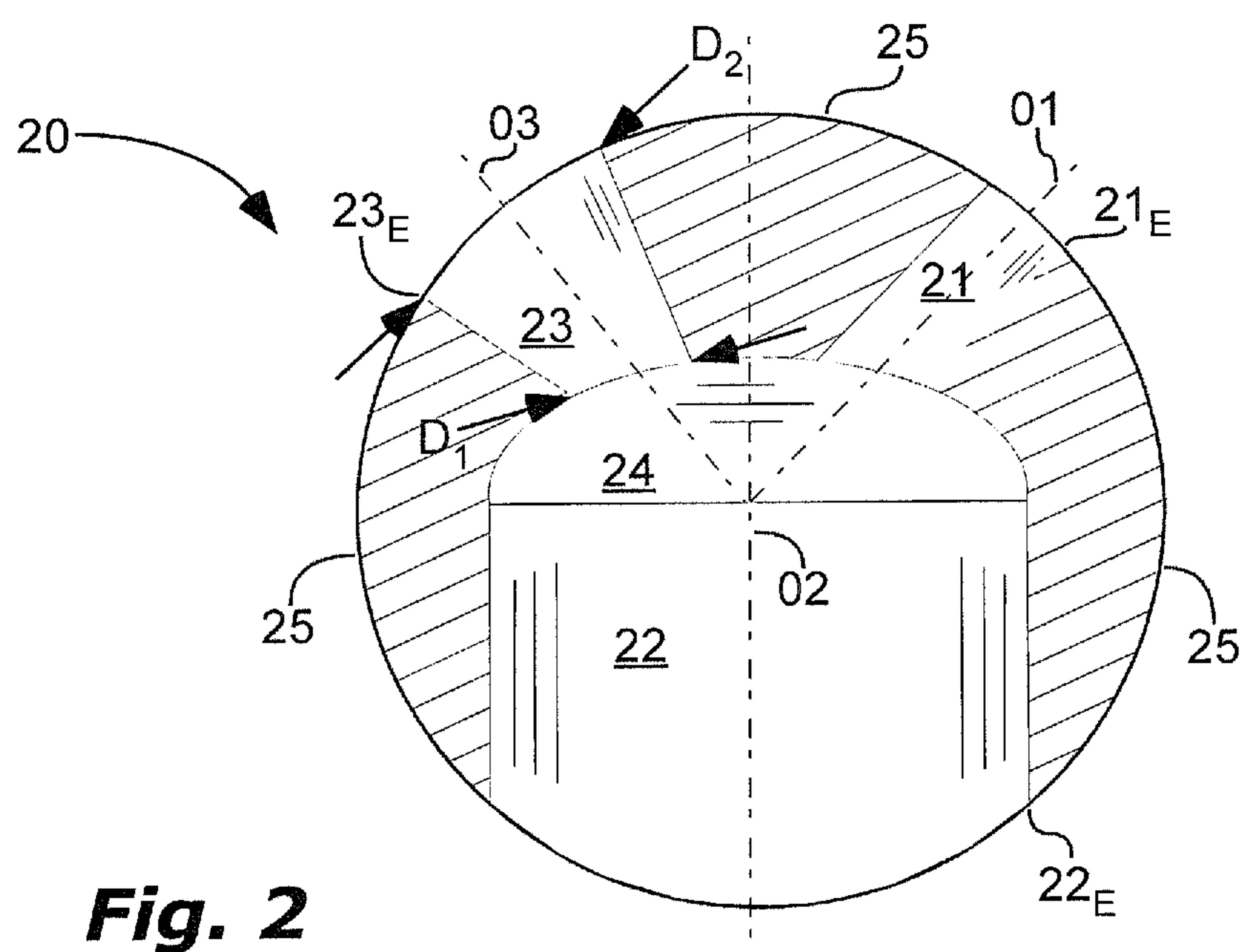
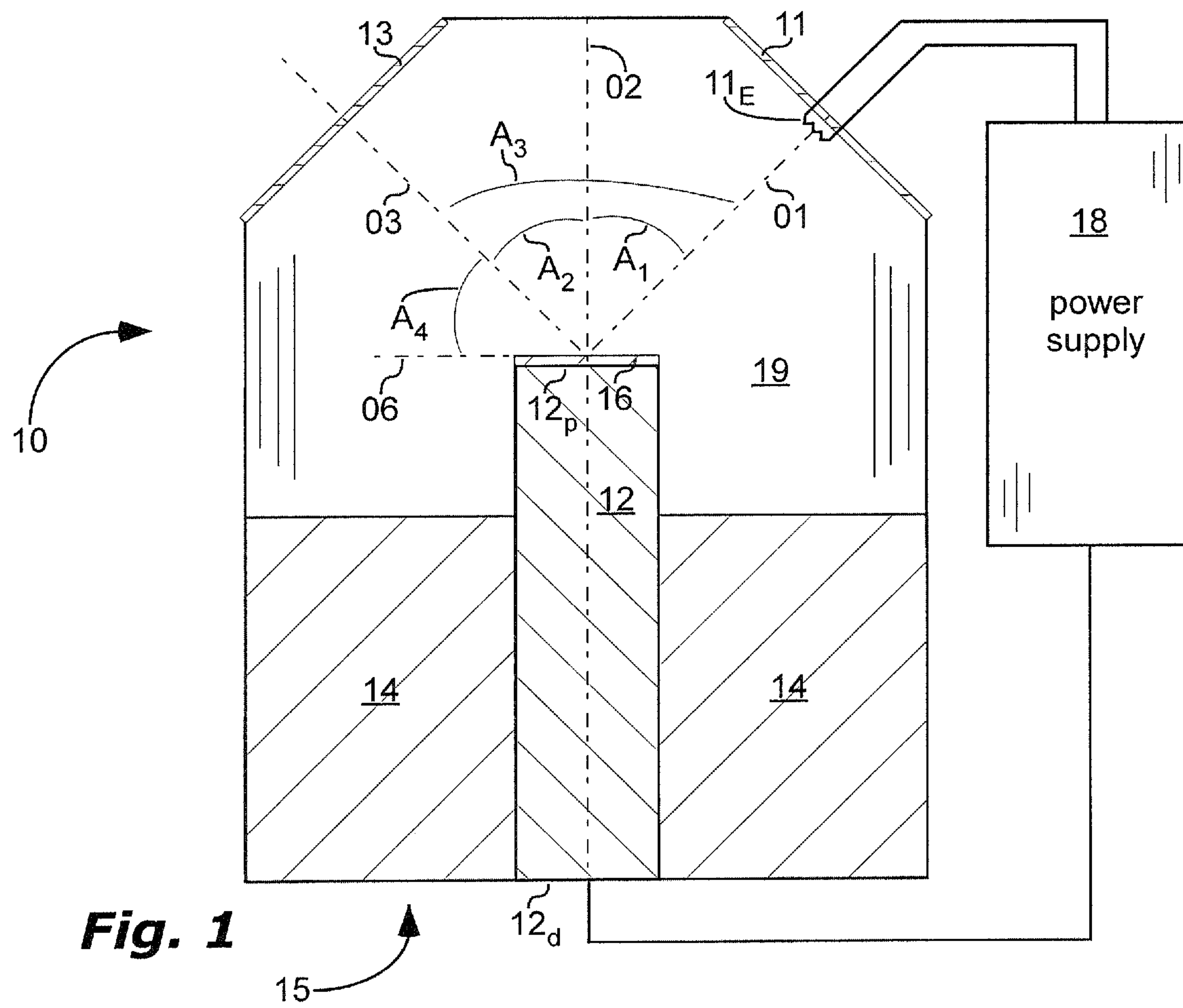
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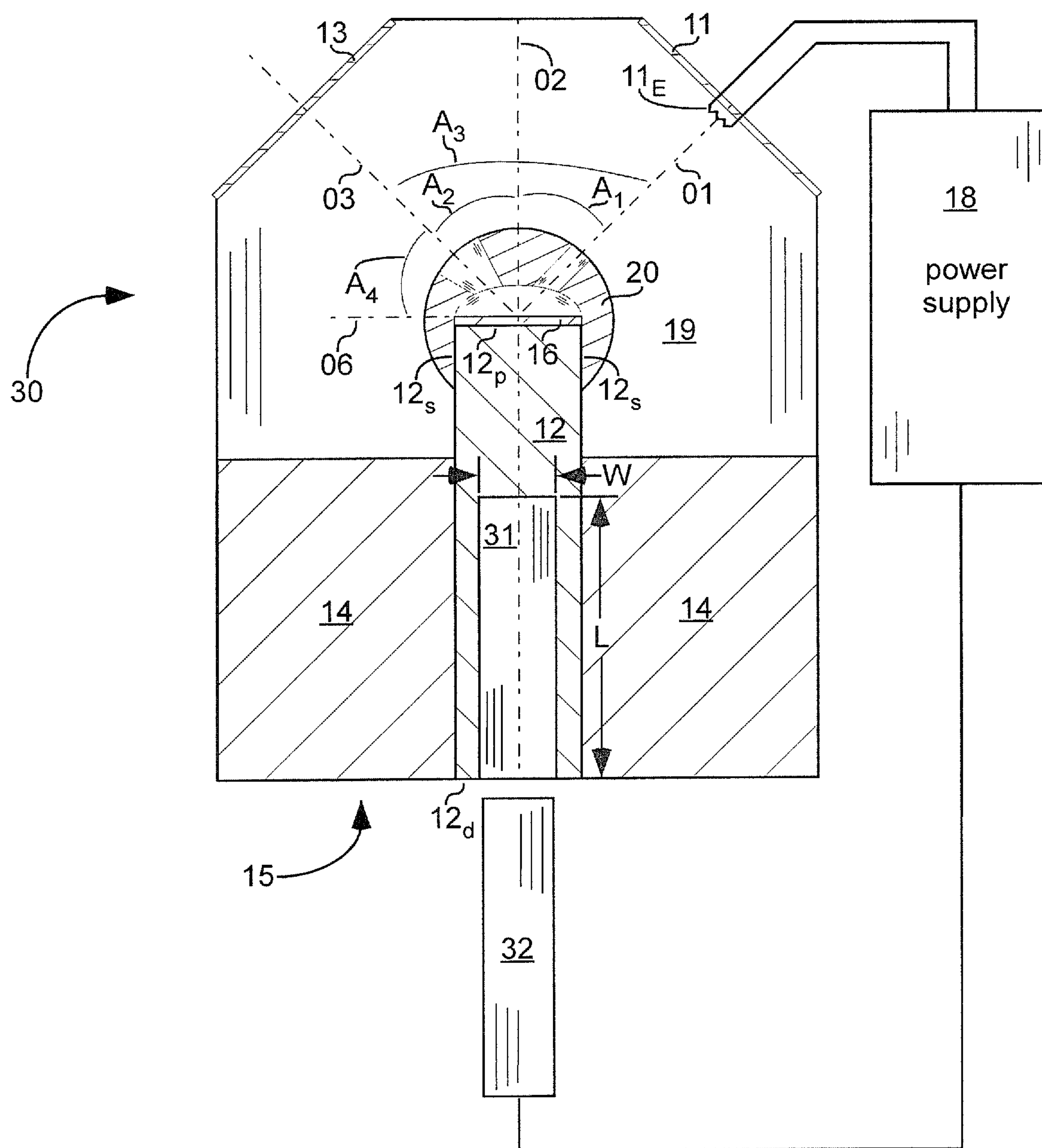


Fig. 3

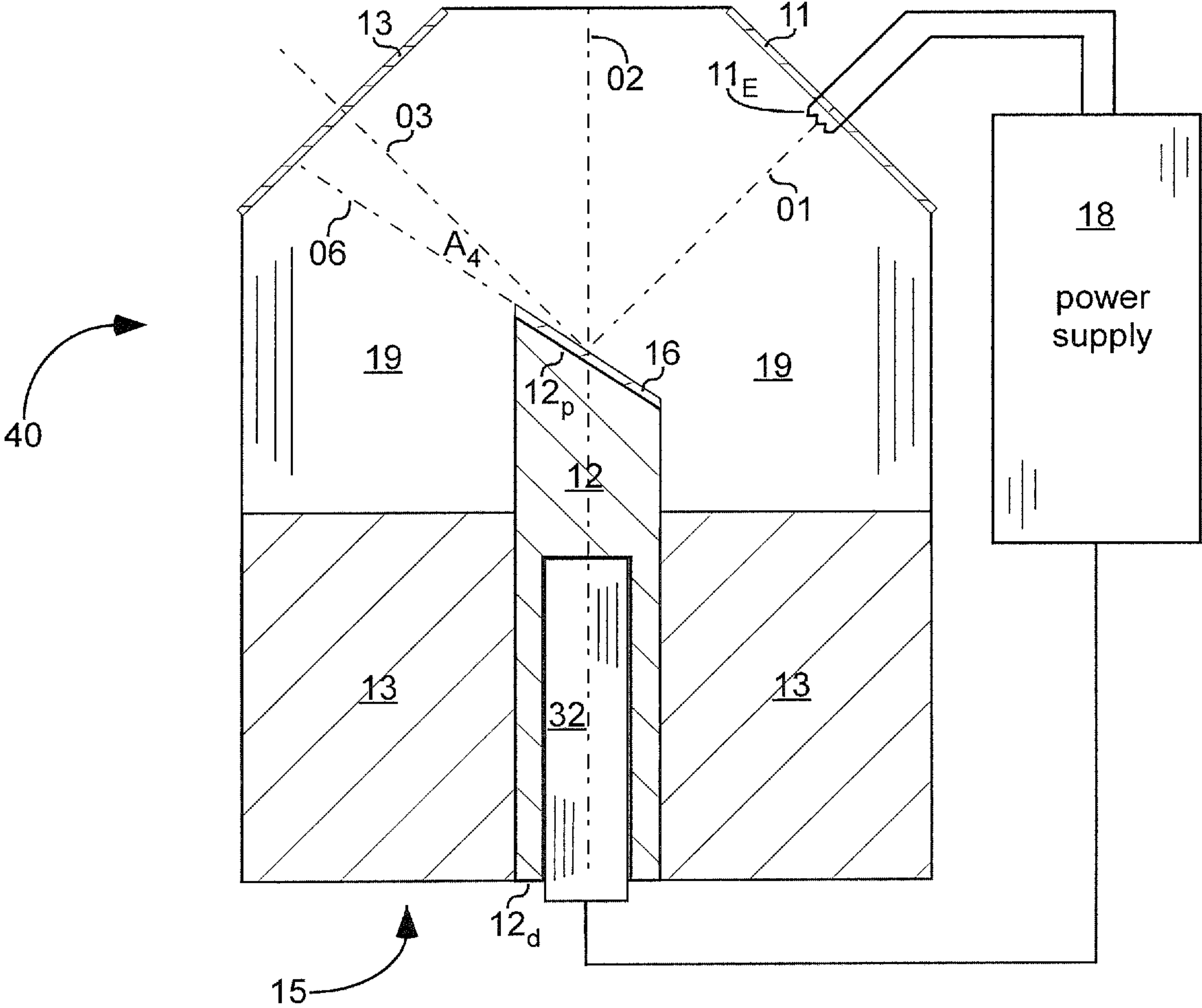


Fig. 4

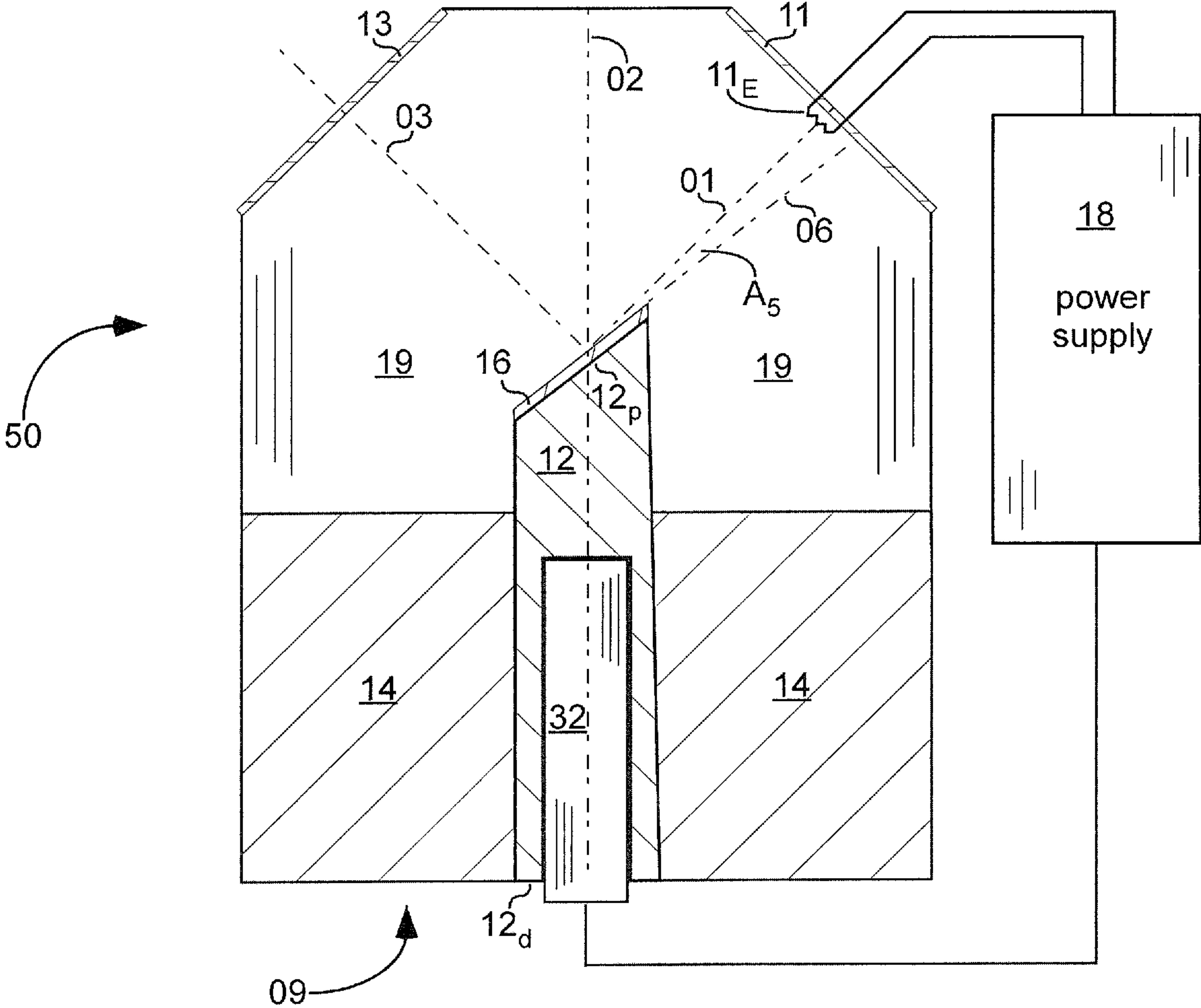


Fig. 5

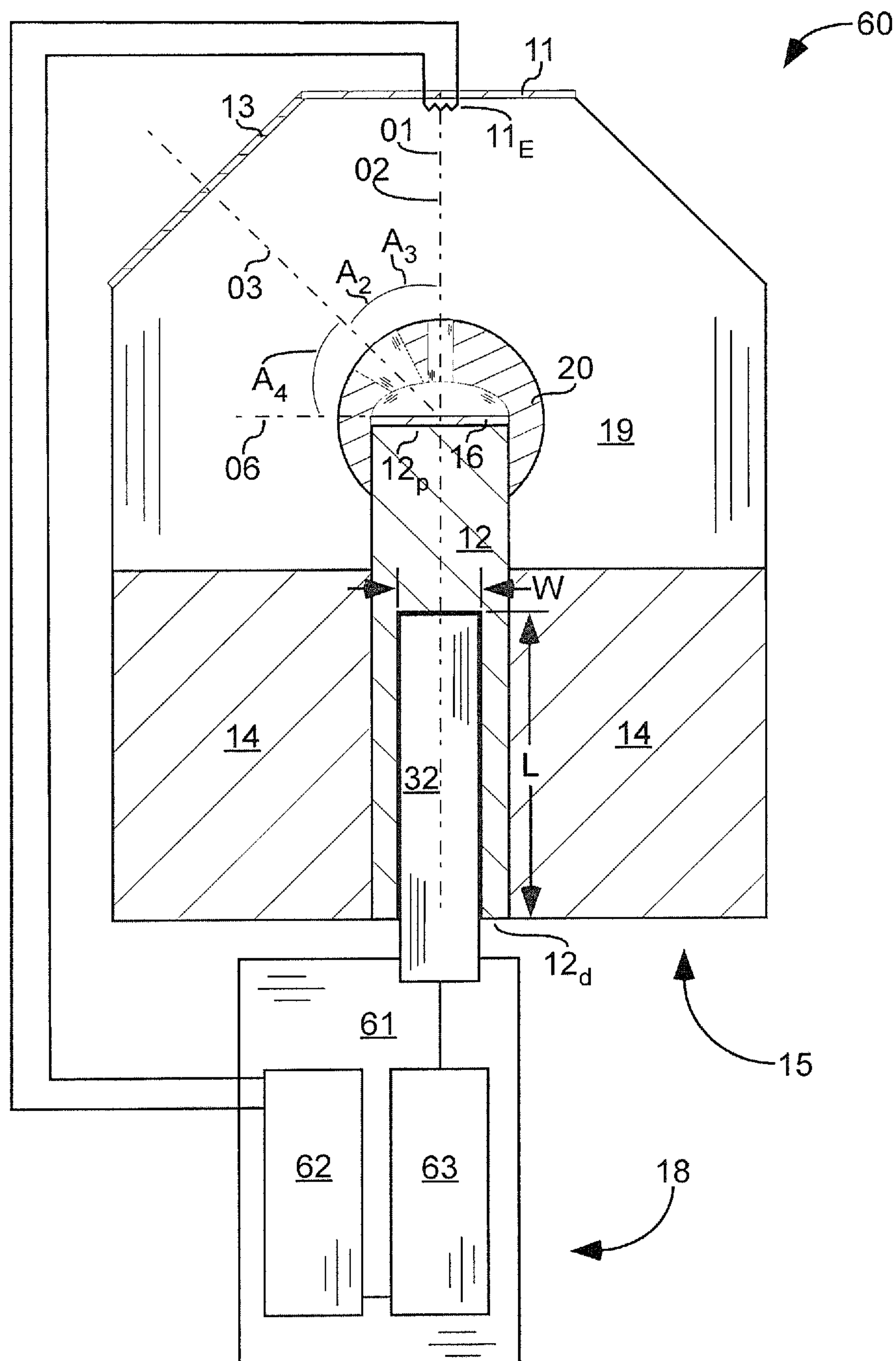


Fig. 6

TRI-AXIS X-RAY TUBE

CLAIM OF PRIORITY

This is a continuation of U.S. patent application Ser. No. 16/144,113, filed on Sep. 27, 2018; which claims priority to U.S. Provisional Patent Application No. 62/577,276, filed on Oct. 26, 2017; which are incorporated herein by reference.

FIELD OF THE INVENTION

The present application is related generally to x-ray sources.

BACKGROUND

In some applications, it can be important for the x-ray tube to be located close to a sample. This is particularly important if small spot size is important (e.g. microfocus x-ray tubes). The structure of the x-ray tube combined with space needed for a detector for analysis of fluoresced x-rays can make it difficult to have the desired distance to the sample. It would be beneficial the distance between the x-ray tube and the sample could be minimized.

In an x-ray tube, in response to impinging electrons from an electron emitter, a target material portion of an anode can emit x-rays in all directions. It can be important for safety considerations to block x-rays emitted in undesired directions. It can be important for cost saving and weight reduction to minimize the weight of material used for blocking such x-rays.

An x-ray source includes an x-ray tube electrically coupled to a power supply. Because the power supply can provide many kilovolts of differential voltage to the x-ray tube, this electrical coupling/electrical connection can be important and careful design is needed for proper electrical connection without undesirable arcing. Furthermore, because the design typically will need to be repeated many times as many such x-ray sources are made, ease of manufacture is another consideration.

SUMMARY

It has been recognized that it would be advantageous to have a minimal distance between the x-ray tube and a sample; to block x-rays emitted by an x-ray tube in undesired directions with minimal weight of material used for blocking such x-rays; and to provide an electrical connection between an x-ray tube and a power supply that is reliable (i.e. not prone to arcing failure) and relatively easy to manufacture. The present invention is directed to various embodiments of x-ray tubes and x-ray sources that satisfy these needs. Each embodiment may satisfy one, some, or all of these needs.

The x-ray tube can comprise a cathode and an anode electrically insulated from one another, the anode including a proximal end closer to the cathode and a distal end farther from the cathode and an x-ray window configured to allow transmission of x-rays, the x-ray window spaced apart from the anode. The cathode can be configured to emit electrons in an electron beam towards the anode. The anode can include target material at the proximal end configured to emit x-rays in response to impinging electrons from the cathode. The x-rays can be emitted in an x-ray beam through an internal cavity of the x-ray tube to and through the x-ray window.

In one embodiment of the x-ray tube in paragraph two of this summary section, an axis along a longest dimension of the anode defines an anode axis, an axis along a center of the electron beam defines an electron-beam axis, and an axis perpendicular to a plane of the x-ray window and along a center of the x-ray beam defines an x-ray axis. An angle between the anode axis and the electron-beam axis can be $\geq 10^\circ$ and $\leq 80^\circ$ and an angle between the anode axis and the x-ray axis can be $\geq 10^\circ$ and $\leq 80^\circ$.

In another embodiment of the x-ray tube in paragraph two of this summary section, the x-ray tube can further comprise a cap on the proximal end of the anode. The cap can include an internal cavity, defining a cap cavity; a first hole, defining an electron-beam hole, extending from an exterior of the cap to the cap cavity along the electron-beam axis; a second hole, defining an anode hole, extending from the exterior of the cap to the cap cavity along the anode axis, the anode located in the anode hole with the target material facing the cap cavity; and a third hole, defining an x-ray hole, extending from the exterior of the cap to the cap cavity along the x-ray axis.

In another embodiment of the x-ray tube in paragraph two of this summary section, the anode can include a hole at the distal end of the anode, defining an anode cavity. The anode cavity can be sized and shaped for insertion of an electrical connector.

BRIEF DESCRIPTION OF THE DRAWINGS
(DRAWINGS MIGHT NOT BE DRAWN TO SCALE)

FIG. 1 is a schematic, cross-sectional side-view of an x-ray source 10 comprising a power supply 18 and an x-ray tube 15, the x-ray tube including an electron-beam axis 01, an anode axis 02, and an x-ray axis 03, in accordance with an embodiment of the present invention.

FIG. 2 is a schematic, cross-sectional side-view of a cap 20 for the anode 12, including a cap cavity 24, an electron-beam hole 21, extending from an exterior 25 of the cap 20 to the cap cavity 24 along the electron-beam axis 01, an anode hole 22 extending from the exterior 25 of the cap 20 to the cap cavity 24 along the anode axis 02, and an x-ray hole 23 extending from the exterior 25 of the cap 20 to the cap cavity 24 along the x-ray axis 03, in accordance with an embodiment of the present invention.

FIG. 3 is a schematic, cross-sectional side-view of an x-ray source 30, similar to the x-ray source 10, further comprising the anode 12 in the anode hole 22 of the cap 20 and an anode cavity 31 in the anode 12 with a matching electrical connector 32, in accordance with an embodiment of the present invention.

FIG. 4 is a schematic, cross-sectional side-view of an x-ray source 40, similar to the x-ray sources 10 and 30, further comprising a face of the anode 12 with the target material 16 tilted towards the an electron emitter 11_E to form an angle A_4 of $<90^\circ$ between a plane 06 of the face of the anode 12 and the x-ray axis 03, in accordance with an embodiment of the present invention.

FIG. 5 is a schematic, cross-sectional side-view of an x-ray source 50, similar to the x-ray sources 10 and 30, further comprising the face of the anode 12 with the target material 16 tilted towards the x-ray window 13 to form an angle A_5 of $<90^\circ$ between the plane 06 of the face of the anode 12 and the electron-beam axis 01, in accordance with an embodiment of the present invention.

FIG. 6 is a schematic, cross-sectional side-view of an x-ray source 60, similar to the x-ray sources 10, 30, 40, and

50, but showing added details of the power supply 18, in accordance with an embodiment of the present invention.

DETAILED DESCRIPTION

As illustrated in FIG. 1, an x-ray source 10 is shown comprising a power supply 18 electrically coupled to an x-ray tube 15 and configured to provide electrical power to the x-ray tube. The power supply 18 can be battery operated, and the x-ray source 10 can be portable with a small weight (e.g. ≤ 1 kg, ≤ 2 kg, ≤ 3 kg, ≤ 4 kg, or ≤ 6 kg). As used herein, the term “kg” means kilogram.

The x-ray tube 15 can comprise a cathode 11 and an anode 12 electrically insulated from one another. This electrical insulation can include a solid or liquid electrically insulative material 14 (e.g. electronic potting compound) and an evacuated internal cavity 19 of the x-ray tube 15. The anode can include a proximal end 12_p closer to the cathode 11 and a distal end 12_d farther from the cathode 11.

An x-ray window 13 can form at least part of an exterior wall of the x-ray tube. The x-ray window 13 can include some or all of the properties (e.g. low deflection, high x-ray transmissivity, low visible and infrared light transmissivity) of the x-ray windows described in U.S. Patent Publication Number 2015/0303024, which is incorporated herein by reference in its entirety. The x-ray window 13 can be spaced apart from the anode 12; thus, the x-ray tube 15 can be a side-window x-ray tube 15. The x-ray window 13 can be electrically insulated from the anode 12. The x-ray window 13, the anode 12, or both can be connected to ground.

The cathode 11 can be configured to emit electrons from an electron emitter 11_E in an electron beam towards the anode 12. The anode 12 can include a target material 16 at the proximal end 12_p configured to emit x-rays in response to impinging electrons from the cathode 11. The x-rays can be emitted in an x-ray beam through an internal cavity of the x-ray tube 10 to and through the x-ray window 13.

The x-ray tube 15 can include an axis along a center of the electron beam, defining an electron-beam axis 01; an axis along a longest dimension of the anode 12, defining an anode axis 02; and an axis along a center of the x-ray beam, which can be perpendicular to a plane of the x-ray window 13, defining an x-ray axis 03. Emitted x-rays can be directed towards a sample. The sample can then fluoresce x-rays that will be collected in and analyzed by an x-ray detector. Space is needed for emission of the x-rays to the sample and the fluoresced x-rays to the detector. If a small x-ray spot on the sample is desirable, then it can be important to minimize this space and thus minimize undesirable expansion of the x-ray beam. Proper selection of angles A₁, A₂, and A₃ between the electron-beam axis 01, the anode axis 02, and the x-ray axis 03 can allow minimization of this space. X-ray sources 10, 30, 40, and 50 in FIGS. 1 and 3-5 with A₁≈45°, A₂≈45°, and A₃≈90° can allow the x-ray tube 15 to be located closer to a sample compared to x-ray source 60 in FIG. 6 with A₁≈0°, A₂≈45°, and A₃≈45°. The x-ray source 60 in FIG. 6 with A₁≈0°, A₂≈45°, and A₃≈45° can be beneficial for other applications and can be preferred for ease of manufacturing.

Examples of angles of the embodiment in FIGS. 1 and 3-5 include: an angle A₁ between the electron-beam axis 01 and the anode axis 02 of $\geq 10^\circ$, $\geq 20^\circ$, $\geq 30^\circ$, or $\geq 40^\circ$ and $\leq 50^\circ$, $\leq 60^\circ$, $\leq 70^\circ$, or $\leq 80^\circ$; an angle A₂ between the anode axis 02 and the x-ray axis 03 of $\geq 10^\circ$, $\geq 20^\circ$, $\geq 30^\circ$, or $\geq 40^\circ$ and $\leq 50^\circ$, $\leq 60^\circ$, $\leq 70^\circ$, or $\leq 80^\circ$; and an angle between the electron-beam axis 01 and the x-ray axis 03 of $\geq 20^\circ$, $\geq 40^\circ$, $\geq 60^\circ$, or $\geq 80^\circ$, and $\leq 100^\circ$, $\leq 120^\circ$, $\leq 140^\circ$, or $\leq 160^\circ$. A₁ plus A₂ can equal A₃.

A cap 20 for the anode 12 is shown in FIG. 2. The cap 20 can include an internal cavity, defining a cap cavity 24. A first hole in the cap 20, defining an electron-beam hole 21, can extend from an exterior 25 of the cap 20 to the cap cavity 24 along the electron-beam axis 01. A second hole in the cap 20, defining an anode hole 22, can extend from the exterior 25 of the cap 20 to the cap cavity 24 along the anode axis 02. A third hole in the cap 20, defining an x-ray hole 23, can extend from the exterior 25 of the cap 20 to the cap cavity 24 along the x-ray axis 03. As shown in FIGS. 3 and 6, the proximal end 12_p of the anode 12 can be located in the anode hole 22 with the target material 16 facing the cap cavity 24. The cap 20 can extend along sides 12_s of the anode from the proximal end 12_p towards the distal end 12_d of the anode 12.

The cap 20 and the anode 12 can comprise material and thicknesses to block x-rays in undesired directions. Because the cap 20 is located very close to the target material 16 and thus close to the source of x-rays, its size can be smaller than shielding that blocks x-rays farther from the source. The anode 12 can block x-rays emitted into the anode hole 22. In order to block the x-rays, the cap 20 and/or the anode 12 can have a high weight percent of materials having a high atomic number. Thus, the cap 20, the anode, or both can have at least 25 weight percent, at least 50 weight percent, at least 75 weight percent, or at least 90 weight percent of materials having an atomic number of at least 42, at least 72, or at least 74. The cap 20 and the anode 12 can have a material composition and thickness to block at least 90%, at least 99%, or at least 99.9% of x-rays emitted from the target material 16 that do not pass through the electron-beam hole 21 or the x-ray hole 23. The cap 20 and the anode 12 can thus block x-rays in all undesired directions except for the electron-beam hole 21. In order to properly block x-rays and avoid a thermal expansion mismatch, a material composition of the cap 20 can be the same as a material composition of the anode 12.

The x-ray hole 23 of the cap 20 can have an expanding size to allow expansion of x-rays that pass through the x-ray hole 23. For example, a largest dimension D₂ of the x-ray hole 23 at the exterior 25 of the cap 20 can be at least 1.2 times larger, at least 1.5 times larger, or at least 2 times larger than a largest dimension D₁ of the x-ray hole 23 at the cap cavity 24. These largest dimensions D₁ and D₂ can be widths or diameters.

The x-ray hole 23 of the cap 20 can shape the emitted x-ray beam. Thus for example, all or part of the x-ray hole 23 can have a rounded shape (e.g. circular, ellipse, etc.), a square shape, or a rectangular shape. Each application of the x-ray sources 10, 30, 40, 50, and 60 described herein may need its own shape of emitted x-ray beam.

Sharp points or sharp edges at the exterior 25 of the cap 20 can result in large voltage gradients adjacent to such points or edges, which can result in malfunctioning of the x-ray tube 15. In order to avoid such large voltage gradients, the exterior 25 of the cap 20 can comprise or consist of smooth curves. For example, the exterior 25 of the cap 20 can have a spherical shape or some other rounded convex shape. Exceptions to the smooth curvature can include an entrance 21_E to the electron-beam hole 21, an entrance 22_E to the anode hole 22, an entrance 23_E to the x-ray hole 23, or combinations thereof.

It can be helpful for the anode 12 to have a low coefficient of thermal expansion for minimal movement of the x-ray spot as the anode changes temperature. Thus for example, the anode 12 can have a coefficient of thermal expansion of ≤ 20 m/(m*K), ≤ 15 m/(m*K), ≤ 12 m/(m*K), or ≤ 10 m/(m*K). It can be helpful for the anode 12 to have a high

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thermal conductivity for transfer of heat away from the target material **16**. Thus for example, the anode **12** can have a thermal conductivity of ≥ 50 W/(m*K), ≥ 100 W/(m*K), ≥ 140 W/(m*K), ≥ 160 W/(m*K), or ≥ 180 W/(m*K).

One potential anode material is tungsten copper, which can be a metal matrix composite. This material combines the high thermal conductivity of copper with the high atomic number and the low coefficient of thermal expansion of tungsten. For example, a material composition of the anode can include at least 50%, at least 60%, at least 70%, at least 80%, or at least 90% tungsten; and/or at least 1%, at least 5%, at least 10%, at least 15%, or at least 20% copper.

A plane **06** of a face of the anode **12** with the target material **16** can be beveled, forming an acute angle with respect to the anode axis **02**, which can change a shape of an x-ray spot on the sample. This shape can be elongated in one of two different directions, each direction at 90° with respect to each other, by changing this angle. For example, as shown in FIG. 4, an angle A_4 between the plane **06** of the face of the anode **12** and the x-ray axis **03** can be $\geq 1^\circ$, $\geq 2^\circ$, $\geq 5^\circ$, or $\geq 15^\circ$ and $\leq 20^\circ$, $\leq 30^\circ$, or $\leq 40^\circ$. As another example, as shown in FIG. 5, for elongation of the spot in a direction 90° from the direction of FIG. 4, an angle A_5 between the plane **06** of a face of the anode **12** with respect to the electron-beam axis **01** can be $\geq 1^\circ$, $\geq 2^\circ$, $\geq 5^\circ$, or $\geq 15^\circ$ and $\leq 20^\circ$, $\leq 30^\circ$, or $\leq 40^\circ$.

As shown in FIG. 3, the anode **12** can include a hole at a distal end of the anode **12** farther from the cathode **11**, defining an anode cavity **31**. The anode cavity **31** can be sized and shaped for insertion of an electrical connector **32**. In FIGS. 4-6, the electrical connector **32** is shown inserted into the anode cavity **31**. The electrical connector **32** provides an electrical coupling to the power supply **18**. The anode **12** can be electrically conductive from the target material **16** to the anode cavity **31** to allow electrical current to flow from the electrical connector **32** in the anode cavity **31** to the target material **16**. The anode cavity **31** and the electrical connector **32** can mate to form a reliable and easy to manufacture electrical connection. The anode cavity **31** and the mating electrical connector **32** can each have a cylindrical shape for easier manufacturing.

A length L (in a direction parallel to the anode axis **02**) and width W (in a direction perpendicular to the anode axis **02**) of the anode cavity **31** can be selected for optimal strength of the anode **12** and area of electrical contact between the anode **12** and the electrical connector **32**. For example, the length L can be ≥ 3 mm, ≥ 3 mm, ≥ 5 mm, or ≥ 10 mm and ≤ 15 mm, ≤ 30 mm, ≤ 100 mm, or ≤ 200 mm. For example, the width W can be ≥ 0.5 mm, ≥ 1 mm, ≥ 2 mm, or ≥ 2.5 mm and ≤ 3.5 mm, ≤ 5 mm, or ≤ 10 mm. As used herein, the term "mm" means millimeter. The actual width W and length L can depend on the actual size of the anode **12**.

As shown in FIG. 6, the power supply **18** can include the electrical connector **32** rigidly connected to and extending from a circuit board **61** into the anode cavity **31** and making electrical contact with the anode **12**. The circuit board **61** can include a voltage multiplier circuit **63** configured to provide electrical power to the electrical connector **32** with a high voltage (e.g. ≥ 1 kilovolt, ≥ 4 kilovolts, or ≥ 10 kilovolts). A control circuit **62** can control and provide input electrical power to the voltage multiplier circuit **63**. An advantage of this design is that the circuit board can provide support for the electrical connector **32** and the x-ray tube **15**; consequently mounting bolts for the circuit board **61** can be avoided or located far from high voltage components, thus reducing the risk of arcing failure. For example, if mounting bolts for the circuit board **61** are used, there can be a distance of ≥ 25 mm, ≥ 40 mm, or ≥ 80 mm between any part of the

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voltage multiplier circuit **63**, having a voltage differential of at least 5000 volts with respect to ground, and a mounting bolt at ground voltage.

An alternative to the electrical connector **32** being rigidly connected to and extending from the circuit board **61** is for the electrical connector **32** to be electrically coupled to the circuit board **61** by a flexible cable. A choice of the rigid mounting or the cable can be made depending on the final use of the x-ray source. A cabled x-ray source can allow the x-ray tube **15** to be inserted into a smaller space, but the cable can add extra weight to the x-ray source, so rigid mounting may be preferable if there is no need to insert the x-ray tube **15** into a smaller space.

What is claimed is:

1. An x-ray tube comprising:

a cathode and an anode electrically insulated from one another, the anode including a proximal end closer to the cathode and a distal end farther from the cathode; an x-ray window configured to allow transmission of x-rays, the x-ray window spaced apart from the anode; the cathode configured to emit electrons in an electron beam towards the anode, the anode including target material at the proximal end configured to emit x-rays in response to impinging electrons from the cathode, the x-rays emitted in an x-ray beam through an internal cavity of the x-ray tube to and through the x-ray window;

an axis along a center of the electron beam defining an electron-beam axis; an axis along a longest dimension of the anode, defining an anode axis; and an axis perpendicular to a plane of the x-ray window and along a center of the x-ray beam, defining an x-ray axis; and the anode including a hole at the distal end, defining an anode cavity, the anode being electrically conductive from the target material to the anode cavity, the anode cavity being sized and shaped for insertion of an electrical connector;

a cap on the anode at the proximal end, the cap including: an internal cavity, defining a cap cavity; a first hole, defining an electron-beam hole, extending from an exterior of the cap to the cap cavity along the electron-beam axis; a second hole, defining an anode hole, extending from the exterior of the cap to the cap cavity along the anode axis, the anode located in the anode hole with the target material facing the cap cavity; and a third hole, defining an x-ray hole, extending from the exterior of the cap to the cap cavity along the x-ray axis.

2. The x-ray tube of claim 1, wherein the anode cavity has a cylindrical shape.

3. The x-ray tube of claim 1, wherein a length of the anode cavity in a direction parallel to the anode axis is between 5 mm and 100 mm and a width of the anode cavity in a direction perpendicular to the anode axis is between 0.5 mm and 8 mm.

4. The x-ray tube of claim 1, wherein a material composition of the anode includes at least 70% tungsten and at least 5% copper.

5. The x-ray tube of claim 1, wherein the anode axis extends from the proximal end to the distal end of the anode.

6. The x-ray tube of claim 5, wherein an angle between the electron-beam axis and the anode axis is $\geq 10^\circ$ and $\leq 80^\circ$ and an angle between the anode axis and the x-ray axis is $\geq 10^\circ$ and $\leq 80^\circ$.

7. The x-ray tube of claim 5, wherein the angle between the electron-beam axis and the anode axis is $\geq 30^\circ$ and $\leq 60^\circ$; the angle between the anode axis and the x-ray axis is $\geq 30^\circ$

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and $\leq 60^\circ$; and an angle between the electron-beam axis and the x-ray axis is $\geq 60^\circ$ and $\leq 120^\circ$.

8. The x-ray tube of claim 5, wherein an angle between a plane of a face of the anode with the target material and the x-ray axis is $\geq 20^\circ$ and $\leq 20^\circ$.

9. The x-ray tube of claim 1, wherein the anode has at least 50 weight percent of materials having an atomic number of at least 42; a coefficient of thermal expansion of $\leq 12 \text{ m/(m}^\circ\text{K)}$; and a thermal conductivity of $\geq 140 \text{ W/(m}^\circ\text{K)}$.

10. The x-ray tube of claim 1, wherein the x-ray hole has an expanding size such that a largest dimension of the x-ray hole at the exterior of the cap is at least 1.5 times larger than a largest dimension of the x-ray hole at the cap cavity.

11. The x-ray tube of claim 1, wherein the exterior of the cap, except for an entrance to the anode hole, consists of smooth curves.

12. The x-ray tube of claim 1, wherein the exterior of the cap has a rounded convex shape.

13. The x-ray tube of claim 1, wherein:

the anode has at least 50 weight percent of materials having an atomic number of at least 42, a coefficient of thermal expansion of $\leq 12 \text{ m/(m}^\circ\text{K)}$, and a thermal conductivity of $\geq 140 \text{ W/(m}^\circ\text{K)}$; and

the cap has at least 50 weight percent of materials having an atomic number of at least 42.

14. The x-ray tube of claim 1, wherein a material composition of the cap is the same as a material composition of the anode.

15. The x-ray tube of claim 1, wherein the x-ray tube forms part of an x-ray source, the x-ray source further comprising a power supply rigidly mounted to the x-ray tube, the power supply including the electrical connector rigidly connected to and extending from a circuit board into the anode cavity and making electrical contact with the anode.

16. The x-ray source of claim 15, further comprising a distance of at least 40 mm between any part of the voltage multiplier circuit, having a voltage differential of at least 5000 volts with respect to ground, and a mounting bolt at ground voltage.

17. The x-ray tube of claim 1, wherein an exterior of the cap has a spherical shape.

18. An x-ray source comprising:

a power supply rigidly mounted to an x-ray tube;

the x-ray tube including a cathode and an anode electrically insulated from one another, the anode including a proximal end closer to the cathode and a distal end farther from the cathode, and an x-ray window configured to allow transmission of x-rays, the x-ray window spaced apart from the anode;

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the cathode configured to emit electrons in an electron beam towards the anode, the anode including target material at the proximal end configured to emit x-rays in response to impinging electrons from the cathode, the x-rays emitted in an x-ray beam through an internal cavity of the x-ray tube to and through the x-ray window;

an axis along a center of the electron beam defining an electron-beam axis; an axis along a longest dimension of the anode, defining an anode axis; and an axis perpendicular to a plane of the x-ray window and along a center of the x-ray beam, defining an x-ray axis;

a cap on the proximal end of the anode, the cap including: an internal cavity, defining a cap cavity; a first hole, defining an electron-beam hole, extending from an exterior of the cap to the cap cavity along the electron-beam axis; a second hole, defining an anode hole, extending from the exterior of the cap to the cap cavity along the anode axis, the anode located in the anode hole with the target material facing the cap cavity; and a third hole, defining an x-ray hole, extending from the exterior of the cap to the cap cavity along the x-ray axis;

an angle between the electron-beam axis and the anode axis being $\geq 30^\circ$ and $\leq 60^\circ$; an angle between the anode axis and the x-ray axis being $\geq 30^\circ$ and $\leq 60^\circ$; and an angle between the electron-beam axis and the x-ray axis being $\geq 60^\circ$ and $\leq 120^\circ$;

the anode having at least 50 weight percent of materials having an atomic number of at least 42, a coefficient of thermal expansion of $\leq 12 \text{ m/(m}^\circ\text{K)}$; and a thermal conductivity of $\geq 140 \text{ W/(m}^\circ\text{K)}$;

the anode including a hole at the distal end, defining an anode cavity, the anode being electrically conductive from the target material to the anode cavity, the anode cavity having a cylindrical shape and being sized and shaped for insertion of an electrical connector; and

the power supply including the electrical connector rigidly connected to and extending from a circuit board into the anode cavity and making electrical contact with the anode.

19. The x-ray tube of claim 18, wherein the x-ray hole has an expanding size such that a largest dimension of the x-ray hole at the exterior of the cap is at least 1.5 times larger than a largest dimension of the x-ray hole at the cap cavity, and the exterior of the cap has a rounded convex shape.

20. The x-ray tube of claim 18, wherein an exterior of the cap has a spherical shape.

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