

US010634741B2

(12) **United States Patent**
Hattersley

(10) **Patent No.:** **US 10,634,741 B2**
(45) **Date of Patent:** **Apr. 28, 2020**

- (54) **MAGNETIC PROBE APPARATUS**
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- (*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 937 days.
- (21) Appl. No.: **12/631,370**
- (22) Filed: **Dec. 4, 2009**
- (65) **Prior Publication Data**
US 2011/0133730 A1 Jun. 9, 2011
- (51) **Int. Cl.**
A61B 17/00 (2006.01)
G01R 33/12 (2006.01)
A61B 5/00 (2006.01)
A61B 5/06 (2006.01)
A61K 49/18 (2006.01)
A61B 5/05 (2006.01)
B82Y 5/00 (2011.01)
- (52) **U.S. Cl.**
CPC *G01R 33/1269* (2013.01); *A61B 5/05* (2013.01); *A61B 5/065* (2013.01); *A61B 5/415* (2013.01); *A61B 5/418* (2013.01); *A61B 5/4312* (2013.01); *A61K 49/1863* (2013.01); *B82Y 5/00* (2013.01); *A61B 2017/00876* (2013.01); *A61B 2562/12* (2013.01)
- (58) **Field of Classification Search**
CPC A61B 5/05; A61B 17/34
USPC 600/407, 409, 422
See application file for complete search history.

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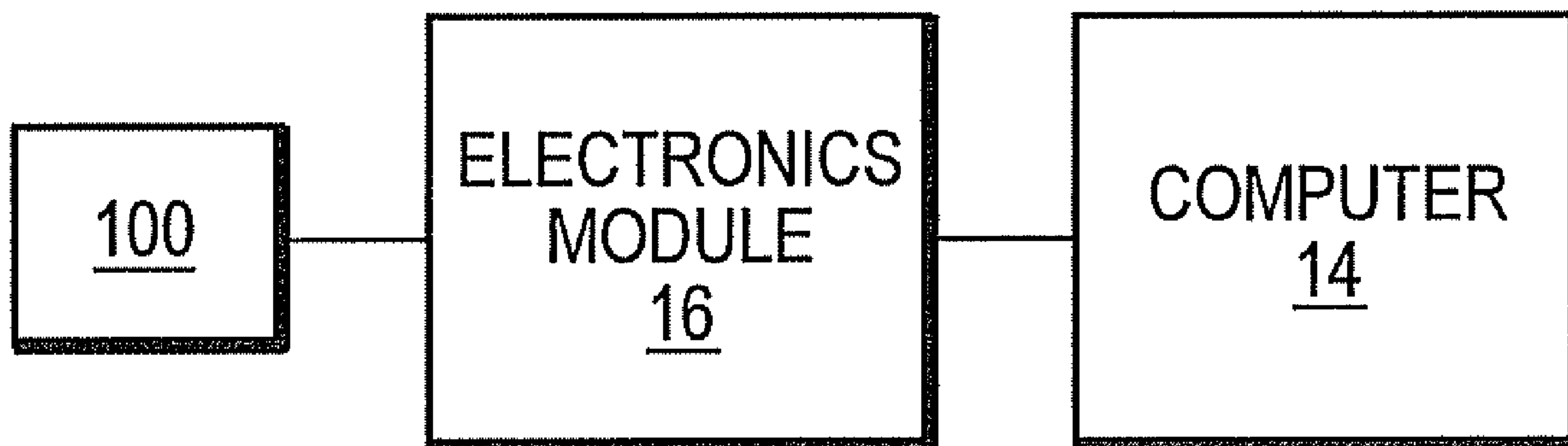
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(57) **ABSTRACT**

A system and method for locating magnetic material. In one embodiment the system includes a magnetic probe; a power module in electrical communication with the magnetic probe to supply current to the magnetic probe; a sense module in electrical communication with the magnetic probe to receive signals from the magnetic probe; and a computer in electrical communication with the power module and the sense module. The computer generates a waveform that controls the supply of current from the power module and receives a signal from the sense module that indicates the presence of magnetic material. The magnetic probe is constructed from a material having a coefficient of thermal expansion of substantially $10^{-6}/^{\circ}\text{C}$. or less and a Young's modulus of substantially 50 GPa or greater. In one embodiment magnetic nanoparticles are injected into a breast and the lymph nodes collecting the particles are detected with the probe and deemed sentinel nodes.

16 Claims, 4 Drawing Sheets

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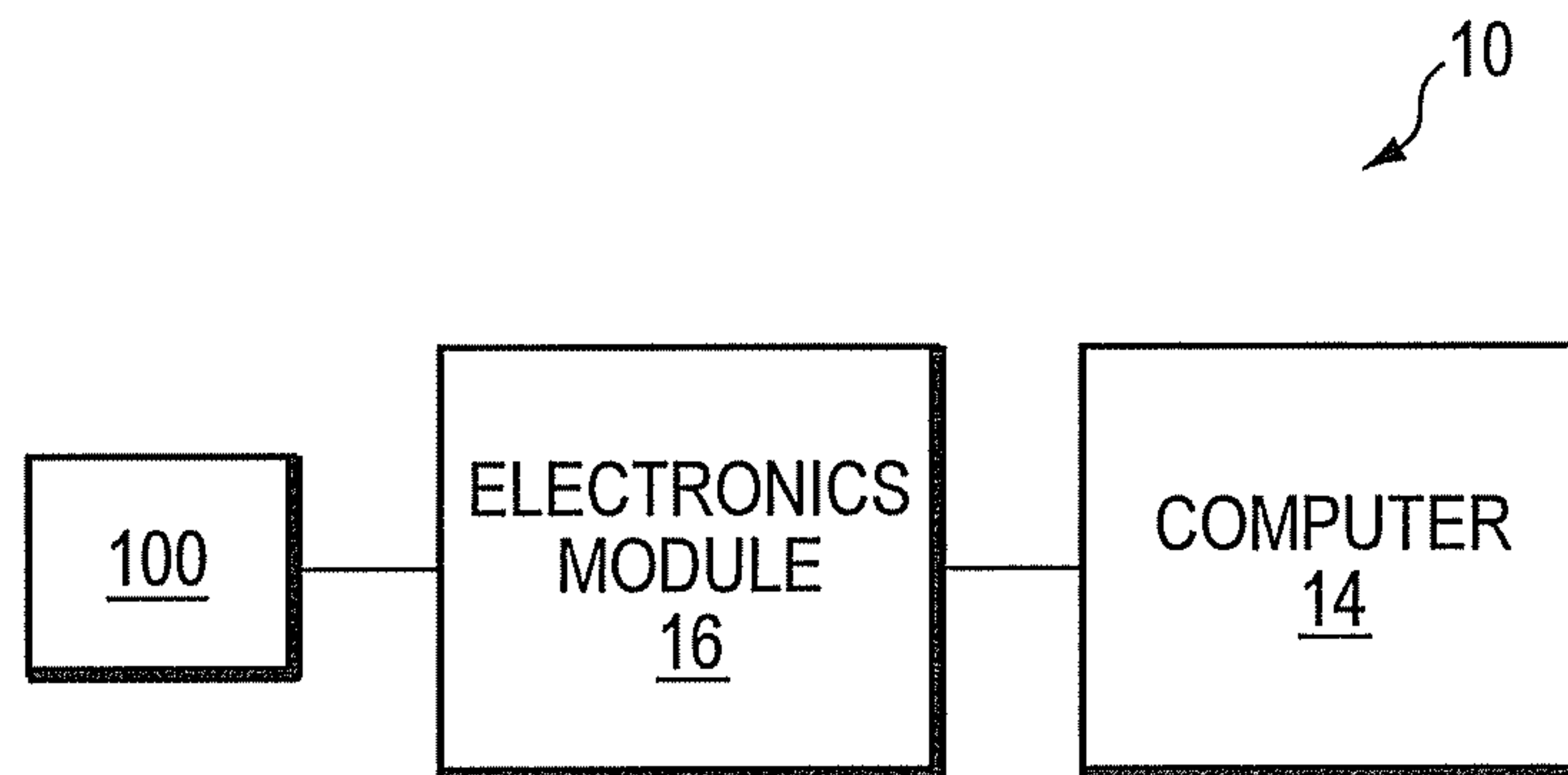


FIG. 1

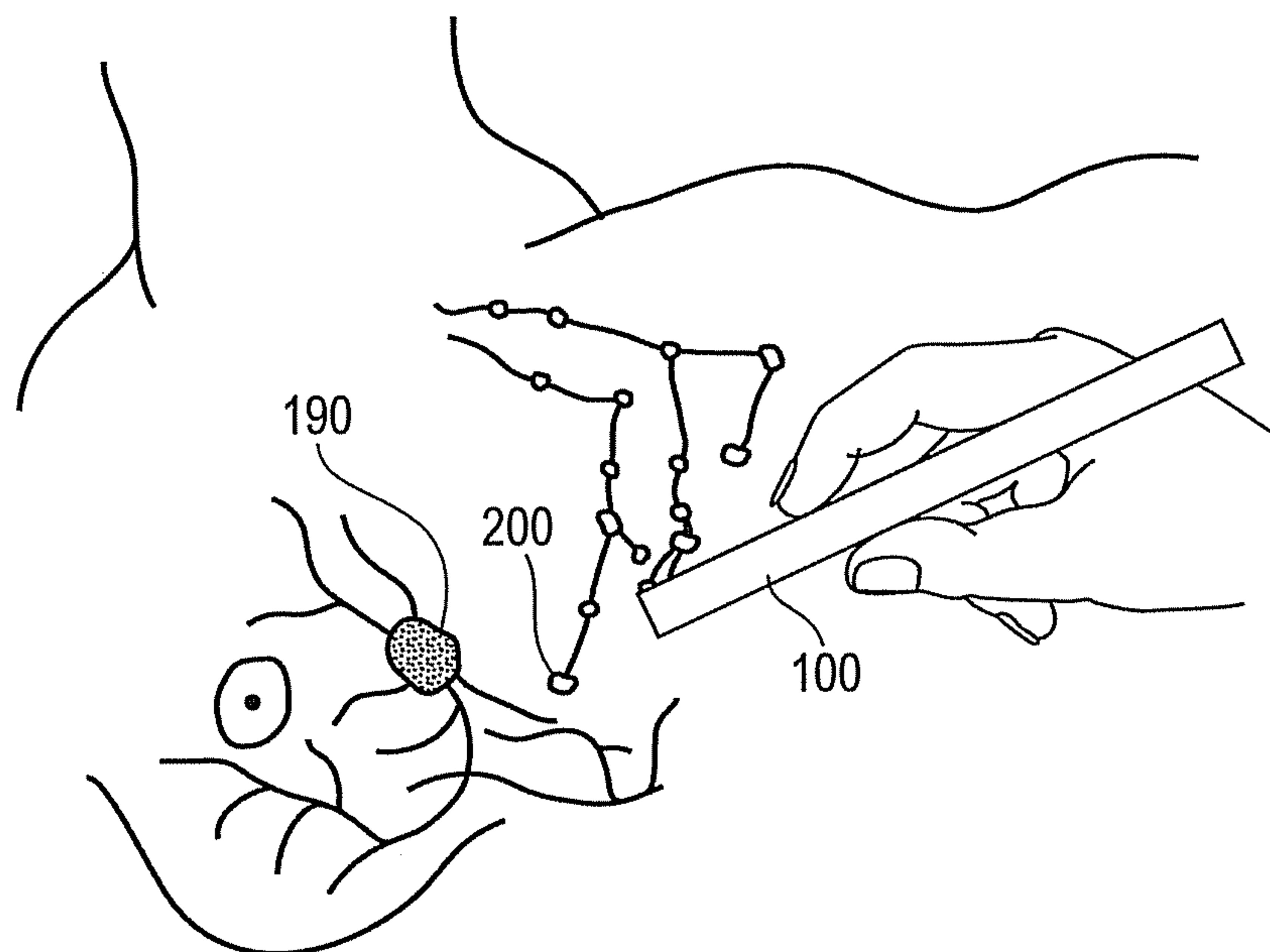


FIG. 4

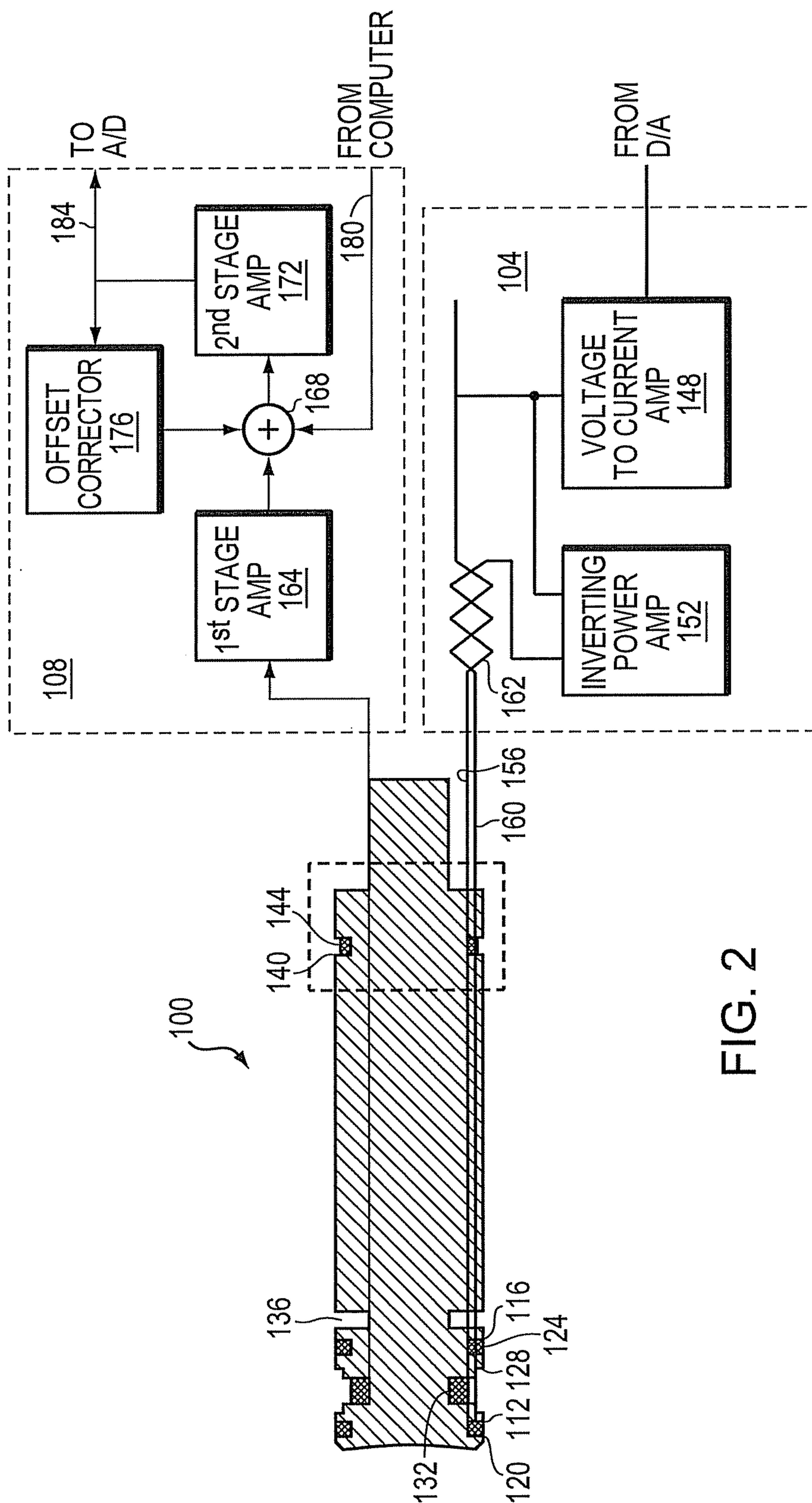


FIG. 2

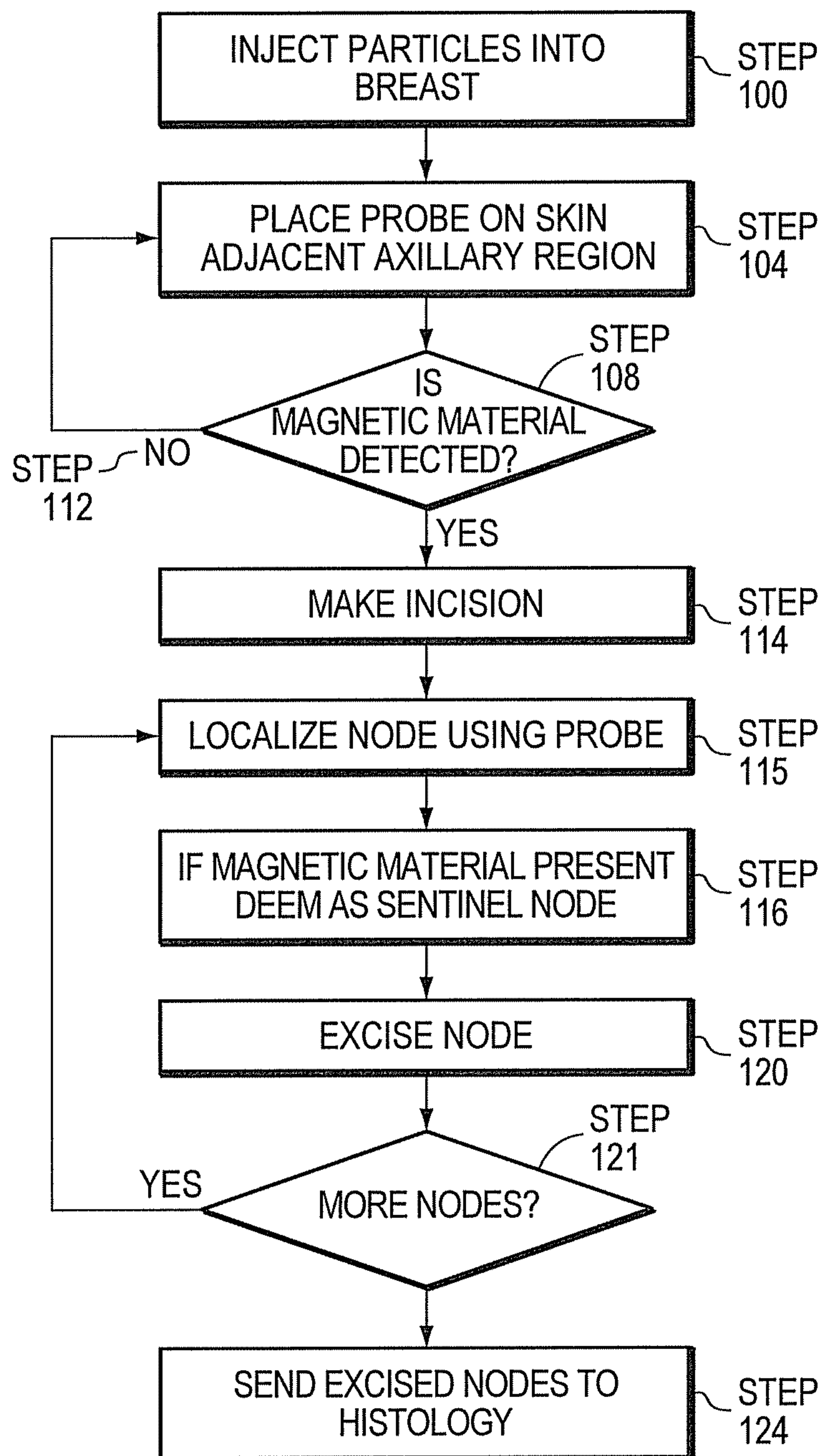


FIG. 3

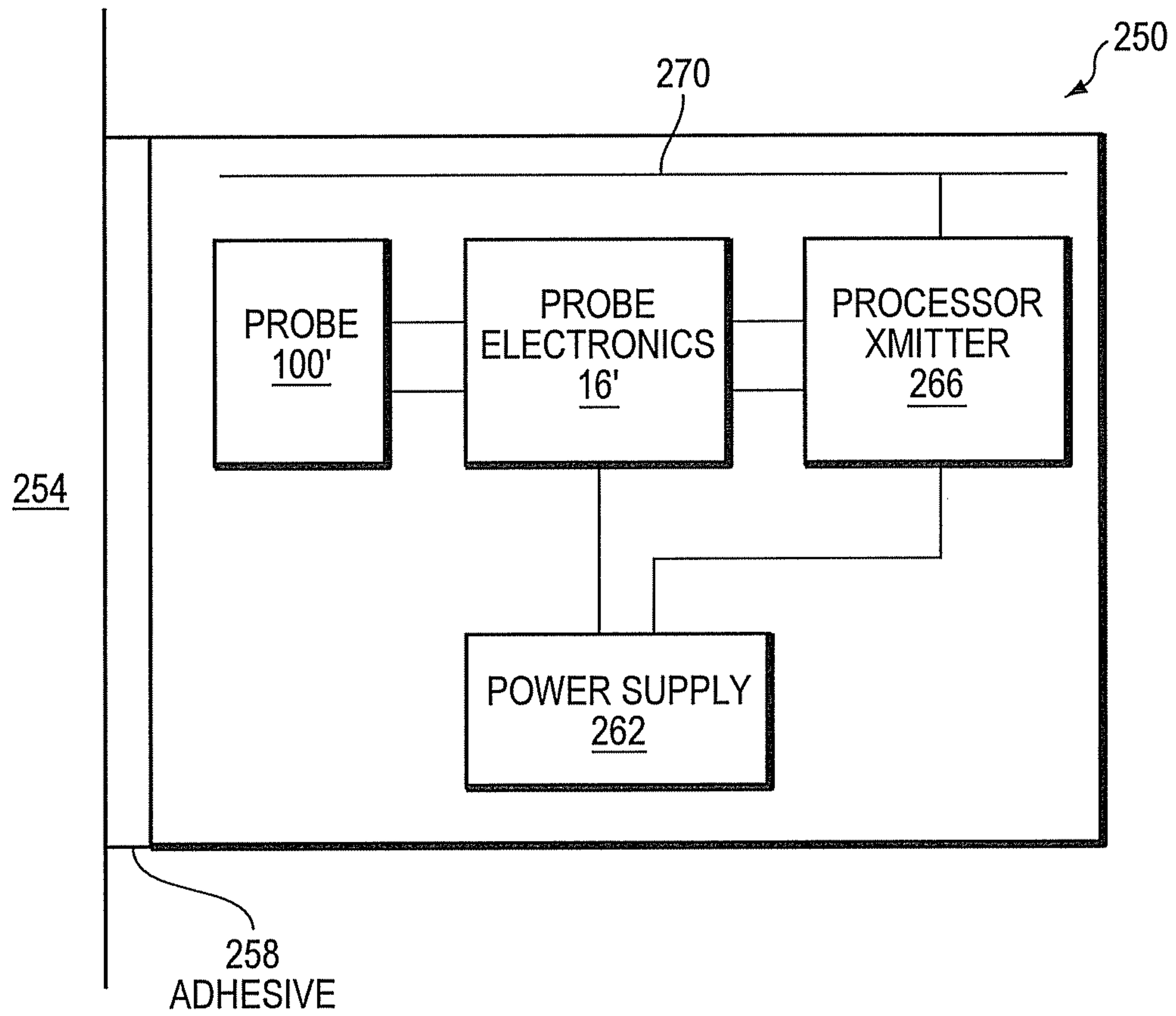


FIG. 5

MAGNETIC PROBE APPARATUS

FIELD OF INVENTION

This invention relates to the field of medical diagnostic devices and more specifically to a device to detect tissues of interest during a surgical procedure.

BACKGROUND

Approximately 1.25 million new cases of breast cancer are diagnosed each year. In a majority of these cases, there is an urgent need for surgery to remove the tumor and to excise the sentinel lymph nodes and inspect them histologically to determine whether the cancer has spread to other sites in the body. The sentinel lymph nodes are the first nodes to receive lymphatic drainage from the tumor. They are called this because they reliably alert the clinician to any cancer spread. A sentinel lymph node biopsy is a standard of care in breast cancer operations today.

Locating sentinel nodes during surgery is difficult. One method for locating the sentinel node is to inject a dark blue dye into the lymphatic system in the breast. The dye then disperses throughout the breast lymphatic system and the surgeon removes any colored nodes. This method is recognized as being error-prone.

An improved method involves injecting a radioactive dye into the lymph nodes. In a similar manner, the dye drains through the lymphatic system and the surgeon then uses a radiation detector to help locate the sentinel nodes. However, the use of radioisotopes presents a significant, and an expensive, logistical burden, because of the need to allocate the time and resources of a nuclear medicine radiologist in addition to the surgeon for what is otherwise a routine operation. Further many patients are reluctant to receive a radioactive injection. These factors become a significant barrier to the widespread adoption of the use of radioisotopes to locate the sentinel nodes.

The present invention overcomes these issues.

SUMMARY OF THE INVENTION

The present invention radically alters the sentinel lymph node protocol through the use of a detection system based on magnetism rather than radiation. The present system combines the magnetic properties of a magnetic nanoparticle suspension with a detector that is significantly more sensitive than other methods that can be used in the environment of an operating theater. In one embodiment the nanoparticles suspension is an FDA approved MRI contrast agent. Although in one embodiment the present invention is directed to locating sentinel lymph nodes, it can be used to detect other magnetic materials both within a body and in other environments.

In one aspect the invention relates to a system for locating magnetic material. In one embodiment the system includes a magnetic probe; a power module in electrical communication with the magnetic probe to supply current to the magnetic probe; a sense module in electrical communication with the magnetic probe to receive signals from the magnetic probe; and a computer in electrical communication with the power module and the sense module. The computer generates a waveform that controls the supply of current from the power module and receives a signal from the sense module that indicates the position of magnetic material. The magnetic probe is constructed from a material having a

coefficient of thermal expansion of substantially $10^{-6}/^{\circ}\text{C}$. or less and a Young's modulus of substantially 50 GPa or more.

In one embodiment the magnetic probe comprises two concentric drive coils positioned on respective sides of a concentric sense coil. The two concentric drive coils are constructed so as to produce a zero magnetic field at the center of the sense coil. In another embodiment the magnetic probe further comprises an optional sense coil positioned away from the drive coils and constructed so as to cancel the ambient magnetic field effects in the sense coil. In yet another embodiment the probe is cylindrical and the drive and sense coils are positioned within respective circumferential grooves in the cylindrical magnetic probe. In still yet another embodiment an additional circumferential groove is constructed in the cylinder to reduce heat conduction.

In another embodiment the magnetic probe comprises two concentric sense coils positioned on respective sides of a concentric drive coil. The two concentric sense coils are constructed so as to produce equal and opposite currents in response to the magnetic field generated by the drive coil.

In another aspect the invention relates to a magnetic probe comprising a probe body having a first end and a second end. The probe body is sized to fit in the hand of a user and comprises a material having a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$. and a Young's modulus of substantially 50 GPa or greater. A sense coil is positioned near the first end of the probe body, and two concentric drive coils are positioned concentric with and on respective sides of the sense coil. The two concentric drive coils are constructed so as to produce a zero magnetic field at the center of the sense coil. In one embodiment the magnetic probe further comprises an optional sense coil positioned away from the drive coils and constructed so as to cancel ambient field effects in the sense coil. In another embodiment the probe is cylindrical and the drive and sense coils are positioned within respective circumferential grooves in the cylindrical magnetic probe. In yet another embodiment an additional circumferential groove is constructed in the cylinder to reduce heat conduction.

In yet another aspect, the invention relates to a magnetic probe comprising a probe body having a first end and a second end. The probe body is sized to fit in the hand of a user and comprises a material having a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$. and a Young's modulus of substantially 50 GPa or greater. A drive coil is positioned near the first end of the probe body and two concentric sense coils are positioned concentric with and on respective sides of the drive coil. The two concentric sense coils are constructed so as to produce equal and opposite currents in response to the magnetic field generated by the drive coil.

In one embodiment the magnetic probe further comprises an optional sense coil positioned away from the drive coils and constructed so as to cancel ambient magnetic field effects in the sense coil. In another embodiment the probe is cylindrical and the drive and sense coils are positioned within respective circumferential grooves in the cylindrical magnetic probe. In yet another embodiment an additional circumferential groove is constructed in the cylinder to reduce heat conduction.

Still yet another aspect of the invention relates to a system for detecting sentinel nodes in a breast lymph system. In one embodiment the apparatus comprises a magnetic probe; a power module in electrical communication with the magnetic probe to supply current to the magnetic probe; a sense module in electrical communication with the magnetic probe to receive signals from the magnetic probe; and a computer

in electrical communication with the power module and the sense module. The computer generates a waveform that controls the supply of current from the power module to the magnetic probe and receives a signal from the sense module that indicates the position of a magnetic particle in the lymph system. The magnetic probe is constructed from a material having a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$. and a Young's modulus of substantially 50 GPa or greater.

In one embodiment the magnetic probe comprises two concentric drive coils positioned on respective sides of a concentric sense coil. The two concentric drive coils are constructed so as to produce a zero magnetic field at the center of the sense coil. In another embodiment the magnetic probe further comprises an optional sense coil positioned away from the drive coils and constructed so as to cancel ambient magnetic field effects in the sense coil. In yet another embodiment the probe is cylindrical and the drive and sense coils are positioned within respective circumferential grooves in the cylindrical magnetic probe. In still yet another embodiment an additional circumferential groove is constructed in the cylinder to reduce heat conduction. In another embodiment the magnetic probe comprises two concentric sense coils positioned on respective sides of a concentric drive coil and wherein the two concentric sense coils are constructed so as to produce equal and opposite currents in response to the magnetic field generated by the drive coil.

In another aspect the invention relates to a magnetic probe including a pair of drive coils and a sense coil. The pair of drive coils and sense coil have different radii. The spacing between the drive coils and the sense coil is such that the rate of change of their mutual inductance with respect to the radius of the larger coil is substantially zero.

In another aspect the invention relates to a magnetic probe having a pair of sense coils, and a drive coil. The pair of sense coils and drive coil have different radii. The spacing between the drive coil and the sense coils is such that the rate of change of their mutual inductance with respect to the radius of the larger coil is substantially zero.

In yet another aspect the invention relates to a method for constructing magnetic probe. The method includes the steps of providing a pair of first coils, and providing a second coil, the pair of first coils and the second coil having different radii, and placing the pair of first coils and the second coil in the probe such that the spacing between the first coils and the second coil is such that the rate of change of their mutual inductance with respect to the radius of the larger coil is substantially zero.

In another aspect the invention relates to a method for detecting sentinel nodes in a breast lymphatic system. In one embodiment the method comprises the steps of: injecting a suspension of magnetic nanoparticles into the tissue of the breast; and scanning the axillary lymph nodes in the armpit, on the same side as the breast, with a magnetic probe. The magnetic probe includes a probe body having a first end and a second end. The probe body is sized to fit in the hand of a user and includes a material having a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$. and a Young's modulus of substantially 50 GPa or more. A sense coil is positioned near the first end of the probe body and two concentric drive coils positioned concentric with and on respective sides of the sense coil. The two concentric drive coils are constructed so as to produce a zero magnetic field at the center of the sense coil. In one embodiment the

magnetic injection is a suspension of magnetic particles. In another embodiment the type of magnetic nanoparticle is a ferum oxide.

BRIEF DESCRIPTION OF THE DRAWINGS

The objects and features of the invention can be better understood with reference to the drawings described below. The drawings are not necessarily drawn to scale; emphasis is instead being placed on illustrating the principles of the invention. In the drawings, numerals are used to indicate specific parts throughout the various views. The drawings associated with the disclosure are addressed on an individual basis within the disclosure as they are introduced.

FIG. 1 is a block diagram of an embodiment of a system constructed in accordance with the invention;

FIG. 2 is a schematic diagram of the probe and electronic components of the embodiment of the system of the system shown in FIG. 1;

FIG. 3 is a flow diagram of an embodiment the method of determining the sentinel nodes utilizing the invention;

FIG. 4 is a drawing of the probe of the system being used to locate a sentinel node; and

FIG. 5 is a block diagram of another embodiment of the system constructed for wireless use.

DETAILED DESCRIPTION

The following description refers to the accompanying drawings that illustrate certain embodiments of the invention. Other embodiments are possible and modifications may be made to the embodiments without departing from the spirit and scope of the invention. Therefore, the following detailed description is not meant to limit the invention. Rather, the scope of the invention is defined by the appended claims.

Referring to FIG. 1, in brief overview, a system constructed in accordance with the teachings of the invention includes a computer 14 having a processor, RAM memory, long term data storage, input/output devices and display; an electronic module 16 containing the power and sensor electronics for the probe and the probe itself 100. In one embodiment the input/output devices include a digital to analog converter and an analog to digital converter.

To maintain the stability of the system, it is necessary in part to provide thermal stability in the probe. This is done with a combination of a material having a combination of low thermal expansion and a high resistance to deformation with a careful positioning of the coils of the probe. Referring to FIG. 2, an embodiment of the electronics and probe components of the system of the invention includes the probe 100, a drive circuit 104 and a sense circuit 108. The probe 100 is generally a cylindrically shaped device sized to fit the hand of a user. In one embodiment the cylinder is about 75 mm long and 20 mm in diameter. In one embodiment the cylinder is made of Zerodur®, (Schott A G, Mainz, Germany) which is an inorganic, non-porous glass ceramic that has a non-directional, isotropic structure. During formation, this glass ceramic is subjected to thermal cycling which converts about 75% of the vitreous material into crystalline quartz. The resulting glass and crystal phases within the material balance such that the thermal expansion coefficient of one form of Zerodur® is of the order $0.02 \times 10^{-6}/^{\circ}\text{C}$. The substantially zero coefficient of expansion maintains the mechanical stability of the probe 100 over a wide temperature range. In addition the glass ceramic material is very stiff having a Young's modulus of 90 GPa. Other

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materials with coefficients of thermal expansion and Young's modulus similar to this material may also be used.

In one embodiment two grooves **112** and **116** are circumferentially formed near the first end of the cylinder body and two substantially identically sized coils of wire **120**, **124** are wound in the grooves. A third groove **128** is also formed in the cylinder substantially midway between and coaxial with the first **112** and second **116** grooves and a third coil **132** wound in that groove **128**. In this embodiment the depth of the third groove **128** is such that the outer surface of the third coil **132** is located at the same depth as the bottom of the first **112** and second **116** grooves and the groove **128** is wider than the other two grooves. In one embodiment the first **120** and second **124** coils are about 2 mm wide; have an inner radius of about 8 mm; and have about 48 turns of wire. The third coil **132** is about 3 mm wide; has an inner radius of about 5 mm and contains about 72 turns of wire.

The size of the coils and their placement relative to each other is selected so that as the coils change shape because of heating, their inductive change is minimized. Unfortunately there are presently no available electrical conductors with zero coefficient of thermal expansion. Tungsten wire offers an improvement over copper wire, reducing the coefficient by a factor of four, but it also suffers from four times the resistivity. For the drive coils the higher resistivity causes increased self-heating, for sense coils the increased resistivity increases the noise, so in the embodiments shown tungsten was not used.

The problem of differential radial expansion of the coils cannot be addressed through material selection, but it can be handled by careful calculation of coil geometry. Consider the coupling (mutual inductance) between a pair of coaxial coils, one of which has a larger radius than the other. If the coils are close together, then the coupling is reduced as the larger coil expands. If the coils are far apart, the coupling increases as the larger coil expands. Thus it is evident that there is a separation at which the coupling is unaffected by small expansions of the larger coil.

With real coils of non-zero radius, length and thickness, the mutual inductance can be calculated numerically as an integral of order 6 over the two coil volumes. Assuming the radii are selected first, the required separation may be determined iteratively. The mutual inductance between two filamentary circuits *i* and *j* is given by the Neumann formula:

$$M_{ij} = \frac{\mu}{4\pi} \oint_{C_i} \oint_{C_j} \frac{ds_i \cdot ds_j}{|R_{ij}|}$$

where R_{ij} is the distance between elements ds_i and ds_j on circuits C_i and C_j , and μ is the magnetic permeability of the material between the filamentary circuits, which for glass ceramics is typically very close to μ_0 , the permeability of free space.

For volume-filling coaxial cylindrical coils, this equation becomes (in cylindrical polar coordinates (r , θ , z):

$M_{ij} =$

$$\frac{\mu}{4\pi} N_i N_j \int_{r_{j0}}^{r_{j1}} \int_{r_{i0}}^{r_{i1}} \int_{z_{j0}}^{z_{j1}} \int_{z_{i0}}^{z_{i1}} \int_{-\pi}^{\pi} \int_{-\pi}^{\pi} \frac{\cos(\theta_i - \theta_j)}{|R_{ij}|} r_i d\theta_i r_j d\theta_j \frac{dz_i}{z_{i1} - z_{i0}} \frac{dz_j}{z_{j1} - z_{j0}} \frac{dr_i}{r_{i1} - r_{i0}} \frac{dr_j}{r_{j1} - r_{j0}}$$

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-continued

where

$$|R_{ij}|^2 = r_i^2 + r_j^2 - 2r_i r_j \cos(\theta_i - \theta_j) + (z_i - z_j)^2$$

and where N_i , N_j are the number of turns on each coil. This equation assumes a uniform current distribution over the coil cross-section, which is valid for low frequency and small wire size so that the skin effect can be neglected.

Given axial symmetry, one integral reduces to the circumference of a circle, leaving the following formula to be integrated numerically:

$$M_{ij} = \mu N_i N_j$$

$$\int_{r_{j0}}^{r_{j1}} \int_{r_{i0}}^{r_{i1}} \int_{z_{j0}}^{z_{j1}} \int_{z_{i0}}^{z_{i1}} r_i r_j \int_0^{\pi} \frac{\cos(\theta_j) d\theta_j}{\sqrt{r_i^2 + r_j^2 - 2r_i r_j \cos(\theta_j) + (z_i - z_j)^2}} \frac{dz_i}{z_{i1} - z_{i0}} \frac{dz_j}{z_{j1} - z_{j0}} \frac{dr_i}{r_{i1} - r_{i0}} \frac{dr_j}{r_{j1} - r_{j0}}$$

It should be understood that the coil coupling is only insensitive to variation in the size of the larger coil, not to variation in the size of the smaller coil. For this technique to be effective, it is therefore necessary that the smaller coil is the central coil within a first order gradiometer made from two equal larger coils. Any change in the radius of the centre coil is balanced by an equal change in coupling to the coils on either side of it. A change in radius of either larger coil is compensated by its correct positioning.

A fourth groove **136** is also formed in the cylinder to reduce the thermal conductivity of the cylinder in use and reduce the amount of any heat generated by the coils **120**, **124** from flowing along the cylinder causing a thermal asymmetry and thereby making the local environment of the two coils **120**, **124** different. Two longitudinal grooves (not shown) are also formed in the surface along the length of the cylinder to provide paths for the wire connections to the various coils.

An optional fifth groove **140** may be formed near the end of the cylinder away from the first groove **112**, and an optional fourth coil **144** formed in the groove **140**. In one embodiment, the fourth coil **144** is about 2 mm wide; has an inner radius of 8 mm and has about 32 turns of wire. Although the fourth coil **144** is larger than the third coil **132**, their area-turns are substantially matched.

In one embodiment the first **120** and second **124** coils are counter wound and connected in series such that when energized by a current, the magnetic fields they produce are substantially cancelled at the center of the third coil **132**. For the purposes of this discussion, unless otherwise stated, the first **120** and second **124** coils are referred to as the drive coils and the third coil **132** as the sense coil. Also the fourth optional coil **144** will also be referred to as an optional sense coil.

Power is supplied to the drive coils **120**, **124** by the drive circuit **104**. The drive circuit includes a voltage to current amplifier **148** and an inverting power amplifier **152**. In one embodiment the computer **14** generates a sine wave of appropriate amplitude and frequency and the digital to analog converter within the computer generates an analog voltage from this generated sine wave. In one embodiment the frequency of the sine wave is 10 kHz. The voltage to current amplifier **148** converts that voltage to a current used

to power the drive coils **120**, **124** through one series connected conductor **156**. In one embodiment the current is 100 mA. The current return conductor **160** is connected to the output terminal of the inverting power amplifier whose input terminal is also connected to the output of the voltage to current amplifier **148**. This configuration produces a balanced +V on one side of the drive coils **120**, **124** and -V on the other side of the drive coils **120**, **124**.

The sense circuit **108** includes a first stage amplifier **164**, a summing junction **168**, a second stage amplifier **172**, and an offset correction circuit **176**. A signal received from the sense coil **132** is the input signal to the first stage sense amplifier **164**. In one embodiment this amplifier has a gain of 250. The output of the first stage gain amplifier **164** is one input to the summing junction **168**. The output of the summing junction **168** is the input to the second stage amplifier **172**. In one embodiment the second stage amplifier has a gain of 400. The output of the second stage amplifier **172** is the input to the offset correction circuit **176** and the input to the analog to digital converter (not shown) connected to the computer **14**.

The offset correction circuit **176** integrates the output of the second stage amplifier **172** and its output is a second input to the summing junction **168**. The output of the offset correction circuit **176** provides a feedback signal in response to a positive offset to generate a negative ramp signal.

The third input to the summing junction **168** is a software controlled balance signal **180**. This signal, which is generated by a second digital to analog converter (not shown) of the computer **10**, is the signal which compensates for any unbalance in the sense coils **120**, **124**. To perform this compensation function the probe **100** is held pointing to open space. The computer **10** generates a compensating balance signal **180** and measures the change of amplitude and phase of the output signal **184**. The computer **10** then calculates the vector (amplitude and phase) for the balance signal **180** necessary to null the output signal **184**.

Thus the balancing process determines the balance phasor required to obtain a near-zero output from the system. Normally balancing starts with the existing value. When starting without a prior value it may be necessary to use a lower drive current initially to avoid saturating the input, and then repeat the balancing at the required drive current.

The system measures the response S_0 at the original balance setting B_0 , then adjusts the balance phasor by a small amount to B_1 and measures the new response S_1 . The coupling from the balance output to the detected input is defined by:

$$X = \frac{S_1 - S_0}{B_1 - B_0}$$

which is the rate of change of the response to balance and therefore the new balance is reached when:

$$B_2 = B_0 - \frac{S_0}{X}$$

Alternatively the computer **10** can generate a balance signal **180**, measure the output signal **184** and modify the balance signal **180** iteratively until the output signal **184** is nulled.

To reduce the noise in the system, the optional sense coil **144** is utilized. This coil **144** is positioned away from the

drive coils **120**, **124** and generally detects the magnetic flux in the operating room and not the magnetic flux from the drive coils **120**. This optional coil **144** can be connected in series with the sense coil **132** such that any ambient magnetic field will produce a current in the optional sense coil **144** that is in opposition to the current that is produced by the ambient magnetic field on the sense coil **132**, thereby canceling the effects of the ambient magnetic field on the probe **100**. It should be noted that when coils are configured to cancel the effects of other coils, the coils canceling each other may be counter wound, or connected in series with their input and output leads reversed.

Further, the functions of the drive coils **120**, **124** and the sense coil **132** can be reversed. If this is done this forms an embodiment in which there are two sense coils **120**, **124** connected in opposition and a drive coil **132** positioned between them. The sense coils **120**, **124** are constructed such that the field of from the drive coil **132** produces a current in each of the sense coils **120**, **124** that is equal and opposite to the current produced in the other sense coil **124**, **120**. The optional sense coil **144** is not needed in this configuration.

To reduce the noise in the system, the power to the coils **120**, **124** and the signals from the sense coil **132** to the sense electronics **108** are each conducted by a twisted quad microphone cable for improved magnetic field rejection. Further the two twisted quad cables are both embedded in a longitudinally flexible yet laterally stiff sheath which prevents the conductors from moving relative to one another.

The output signal **184** from the sense circuit **108** is digitized by the computer's **14** analog to digital converter to provide an output time series. This time series is correlated to the output series generated by the computer **14**.

In particular, detection of the magnetic particles involves correlating the sampled input waveform with two sinusoidal reference waveforms, one in phase with the drive and one in quadrature. The result is a phasor; a complex number giving the amplitude and phase of the probe response:

$$S = \frac{2 \sum_N C_i V_i}{N} + i \frac{2 \sum_N S_i V_i}{N}$$

where V_i is the sampled input voltage and C_i and S_i are sampled cosine and sine waves respectively, and the input is processed in sections of N samples.

It is possible to use the amplitude $|S|$ as the system indication, in which case both magnetic and conductive materials are detected, or to use the dot product with a discrimination phasor to detect only the magnetic component. This works because the eddy current induced in a conductive material is in quadrature with the applied field, while the magnetization of a magnetic material at low frequency is in phase with the applied field. Thus the system can be used not only for detecting magnetic materials but also conductive materials.

As the probe **100** is positioned closer to a node with magnetic particles, the results are displayed, in one embodiment, as an audible sound of increasing frequency and a graphics display of counts proportional to the detected field.

Referring to FIG. 3, during a surgical operation, a surgeon injects (Step **100**) the breast with a suspension of magnetic nanoparticles near a tumor **190** (FIG. 4). In one embodiment the nanoparticles are those used as an MRI contrast agent. Feridex® (Bayer HealthCare Pharmaceuticals, Montville, N.J.) or Endorem™ (Guerbet, Paris, France) are ferum

oxides used generally as an MRI contrast agent which are suitable for the magnetic detection purpose.

After a period of time the suspension drains into the axillary lymphatic system on the same side as the breast. The surgeon then places (Step 104, FIG. 3) the probe 100 on the surface of the skin, attempting to localize a lymph node 200 (FIG. 4) by determining if magnetic particles are detected (Step 108). If not (Step 112) the surgeon continues to search for a node by placing the probe 100 in another location on the surface of the skin and the process repeats. If a magnetic region is detected, the surgeon then makes an incision (Step 114) and attempts to localize the node with magnetic particles using the probe (Step 115). If the node has accumulated the magnetic nanoparticles, it is deemed (Step 116) a sentinel node. The node is then excised (Step 120). The surgeon then looks for additional nodes (Step 121) which may also be sentinel nodes and when complete sends the excised nodes for histological examination for evidence of cancer (Step 124).

Referring to FIG. 5, the system of the invention may be used to study the long term properties of magnetic materials either in a biological context or otherwise. In one embodiment the probe 100' of the invention is reduced in size and rather than being held by a user is placed in a small capsule 250 that is attached to the object of interest 254 by an adhesive 258. The capsule 250 also houses a power supply battery 262, the probe electronics 16', a microprocessor and transmitter 266 and an antenna 270. The output of the probe electronics 16' is digitized by the microprocessor 266 and the data transmitted using the antenna 270 to a receiving computer system (not shown). This embodiment for example is useful in tracking the behavior of magnetic particles without requiring that the patient or object be tethered to the computer system 14 by wires.

It is to be understood that the figures and descriptions of the invention have been simplified to illustrate elements that are relevant for a clear understanding of the invention, while eliminating, for purposes of clarity, other elements. Those of ordinary skill in the art will recognize, however, that these and other elements may be desirable. However, because such elements are well known in the art, and because they do not facilitate a better understanding of the invention, a discussion of such elements is not provided herein. It should be appreciated that the figures are presented for illustrative purposes and not as construction drawings. Omitted details and modifications or alternative embodiments are within the purview of persons of ordinary skill in the art.

It can be appreciated that, in certain aspects of the invention, a single component may be replaced by multiple components, and multiple components may be replaced by a single component, to provide an element or structure or to perform a given function or functions. Except where such substitution would not be operative to practice certain embodiments of the invention, such substitution is considered within the scope of the invention.

The examples presented herein are intended to illustrate potential and specific implementations of the invention. It can be appreciated that the examples are intended primarily for purposes of illustration of the invention for those skilled in the art. There may be variations to these diagrams or the operations described herein without departing from the spirit of the invention. For instance, in certain cases, method steps or operations may be performed or executed in differing order, or operations may be added, deleted or modified.

Furthermore, whereas particular embodiments of the invention have been described herein for the purpose of illustrating the invention and not for the purpose of limiting

the same, it will be appreciated by those of ordinary skill in the art that numerous variations of the details, materials and arrangement of elements, steps, structures, and/or parts may be made within the principle and scope of the invention without departing from the invention as described in the

Variations, modification, and other implementations of what is described herein will occur to those of ordinary skill in the art without departing from the spirit and scope of the invention as claimed. Accordingly, the invention is to be defined not by the preceding illustrative description, but instead by the spirit and scope of the following claims.

What is claimed is:

1. A magnetic probe comprising:

a handheld probe body comprising a first drive coil having a first radius, a second drive coil having a second radius and a non-porous ceramic material, the handheld probe body having an axis, wherein the handheld probe body is cylindrically shaped; and

a sense coil positioned between the first drive coil and the second drive coil, the sense coil having a third radius, wherein the third radius is larger than the first radius and the second radius, wherein center of the first drive coil, center of the second drive coil, and center of sense coil are disposed along the axis of the handheld probe body, wherein the first drive coil is disposed in a first groove, wherein the second drive coil is disposed in a second groove, wherein the sense coil is disposed in a third groove,

wherein each of the first groove, the second groove and the third groove are circumferentially formed in the non-porous ceramic material,

wherein an axial spacing between the first drive coil and the sense coil is such that while the first radius of the first drive coil and the third radius of the sense coil expand in response to heating change in mutual inductance between the sense coil and the first drive coil is inherently zero.

2. A magnetic probe comprising:

a handheld probe body comprising a first sense coil having a first radius and a second sense coil having a second radius and a non-porous ceramic material, the handheld probe body having an axis, wherein the handheld probe body is cylindrically shaped; and

a drive coil positioned between the first sense coil and the second sense coil, the drive coil having a third radius, wherein the third radius is smaller than the first radius and the second radius, wherein center of the first sense coil, center of the second sense coil, and center of drive coil are disposed along the axis of the handheld probe body, wherein the first sense coil is disposed in a first groove, wherein the second sense coil is disposed in a second groove, wherein the drive coil is disposed in a third groove,

wherein each of the first groove, the second groove and the third groove are circumferentially formed in the non-porous ceramic material,

wherein an axial spacing between the drive coil and the first sense coil is such that while the first radius of the first sense coil and the third radius of the drive coil expand in response to heating change in mutual inductance between the first sense coil and the drive coil is inherently zero.

3. The magnetic probe of claim 1 wherein said the first drive coil and the second drive coil form a first order gradiometer.

4. The magnetic probe of claim 2 wherein the first sense coil and the second sense coil form a first order gradiometer.

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5. The magnetic probe of claim 1 wherein the probe body has a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$.

6. The magnetic probe of claim 2 wherein the probe body has a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$.

7. The magnetic probe of claim 1 the probe body having a Young's modulus of 50 GPa or greater.

8. The magnetic probe of claim 2 the probe body having a Young's modulus of 50 GPa or greater.

9. A magnetic probe comprising:

a handheld probe body having a first end and a second end, the handheld probe body comprising

a non-porous ceramic material;

a drive coil having a first radius; and

a sense coil having a second radius, the sense coil and the drive coil connected to a conductor, wherein the conductor extends from the first end, wherein the first radius is larger than the second radius the handheld probe body having an axis, wherein the drive coil and the sense coil are wound relative to a shared surface of the probe body, wherein the drive coil is disposed in a first groove, wherein the sense coil is disposed in a second groove,

wherein the handheld probe body is cylindrically shaped and the drive coil and sense coil are positioned near the second end,

wherein each of the first groove and the second groove are circumferentially formed in the non-porous ceramic material,

wherein an axial spacing between the drive coil and the sense coil is such that while the first radius and the second radius expand in response to heating change in mutual inductance between the sense coil and the drive coil is inherently zero.

10. The magnetic probe of claim 1 wherein the first drive coil, the second drive coil, and the sense coil are wound relative to the axis and further comprising a display in electrical communication with one or more of the coils, the display configured to display changes in detecting magnetic particles in a patient as position of handheld probe body changes.

11. The magnetic probe of claim 2 wherein the first sense coil, the second sense coil, and the drive coil are wound

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relative to the axis and further comprising a display in electrical communication with one or more of the coils, the display configured to display changes in detecting magnetic particles in a patient as position of handheld probe body changes.

12. The magnetic probe of claim 9 wherein the handheld probe body has a coefficient of thermal expansion less than or equal to $10^{-6}/^{\circ}\text{C}$.

13. The magnetic probe of claim 9 probe body having a Young's modulus of 50 GPa or greater.

14. The magnetic probe of claim 3 wherein the first drive coil and the second drive coil are constructed so as to produce a zero magnetic field at the center of the sense coil.

15. The magnetic probe of claim 4 wherein the first and second sense coils are constructed so as to produce equal and opposite currents in response to magnetic field generated by the drive coil.

16. A method of reducing, in a hand held magnetic probe comprising a first drive coil having a first radius, a second drive coil having a second radius and a sense coil having a third radius, a change in mutual inductance from coil heating, the method, comprising:

arranging the first drive coil, the second drive coil and the sense coil so as to be spaced apart coaxially, concentrically relative to an axis of a cylindrically shaped non-porous ceramic material, and such that the sense coil is disposed between the first drive coil and the second drive coil and wherein the first drive coil is disposed in a first groove, wherein the second drive coil is disposed in a second groove, wherein the sense coil is disposed in a third groove;

sizing the first radius, the second radius, the third radius and relative position of the first drive coil and the sense coil such that as each respective coil changes shape in response to heating change in mutual inductance between each respective coil is minimized to be inherently zero, wherein the third radius is smaller than the first radius and the second radius;

detecting nanoparticles in the patient using the sense coil, wherein the third groove is circumferentially formed in the non-porous ceramic material; and

displaying, using a display in electrical communication with the probe, results of detecting nanoparticles.

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