



(12) **United States Patent**
Truschel et al.

(10) **Patent No.:** **US 10,518,050 B2**
(45) **Date of Patent:** **Dec. 31, 2019**

(54) **SYNCHRONOUS AIRWAY PRESSURE
RELEASE VENTILATION**

(58) **Field of Classification Search**

CPC A61M 16/00; A61M 16/0003; A61M
16/0006; A61M 16/0009; A61M 16/0057;

(Continued)

(71) Applicant: **KONINKLIJKE PHILIPS N.V.**,
Eindhoven (NL)

(56) **References Cited**

(72) Inventors: **William Anthony Truschel**, Oakmont,
PA (US); **John Seymour**, New
Kensington, PA (US)

U.S. PATENT DOCUMENTS

4,773,411 A 9/1988 Downs
5,513,631 A 5/1996 McWilliams

(Continued)

(73) Assignee: **Koninklijke Philips N.V.**, Eindhoven
(NL)

FOREIGN PATENT DOCUMENTS

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 826 days.

WO WO9945989 A1 9/1999
WO WO2011057362 A1 5/2011
WO WO2011070472 A1 6/2011

Primary Examiner — Josph D. Boecker

(74) *Attorney, Agent, or Firm* — Michael W. Haas

(21) Appl. No.: **14/897,019**

(22) PCT Filed: **Jun. 5, 2014**

(86) PCT No.: **PCT/IB2014/061965**

§ 371 (c)(1),

(2) Date: **Dec. 9, 2015**

(87) PCT Pub. No.: **WO2014/199264**

PCT Pub. Date: **Dec. 18, 2014**

(65) **Prior Publication Data**

US 2016/0151594 A1 Jun. 2, 2016

Related U.S. Application Data

(60) Provisional application No. 61/833,552, filed on Jun.
11, 2013.

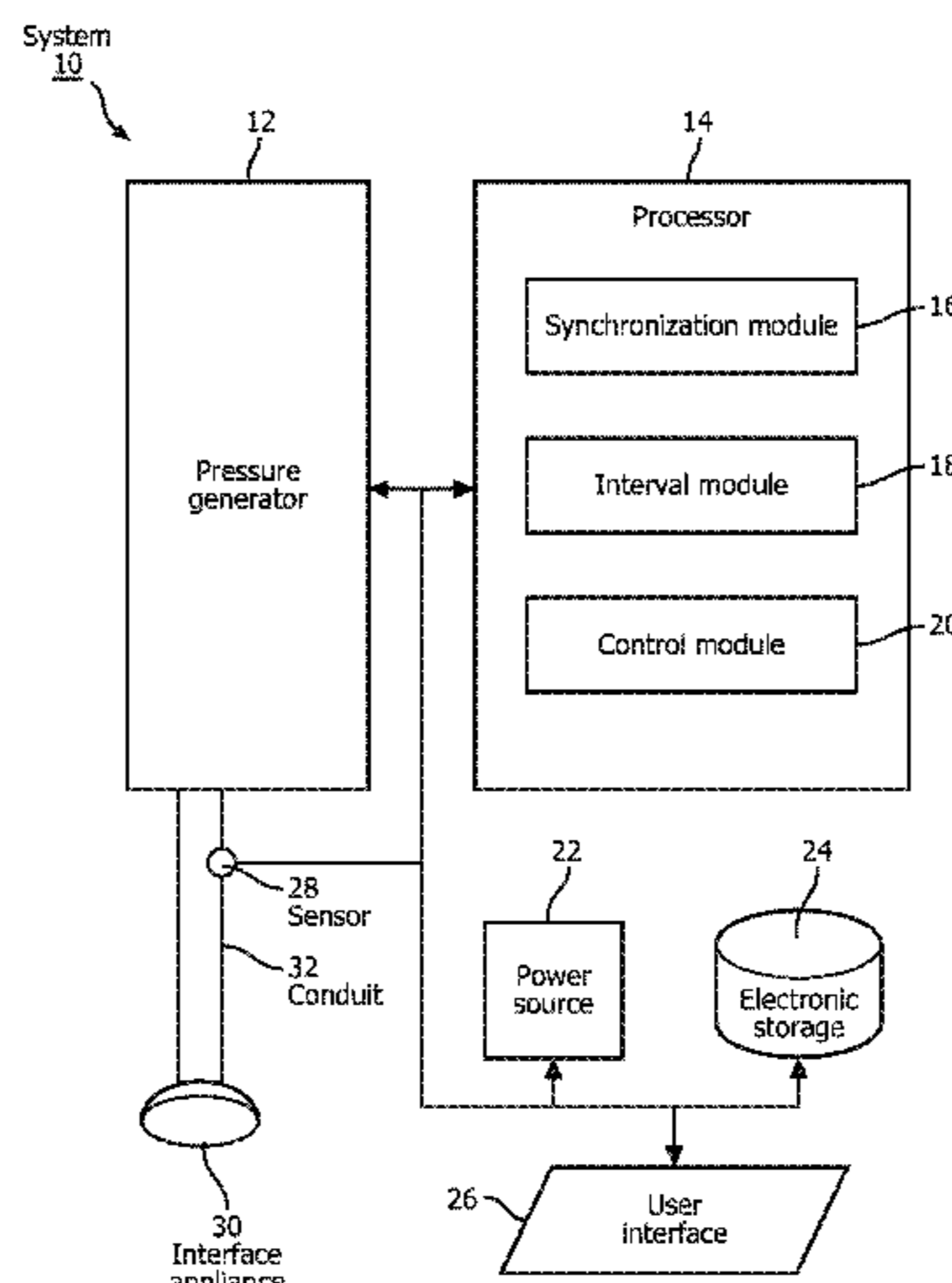
(51) **Int. Cl.**
A61M 16/00 (2006.01)

(52) **U.S. Cl.**
CPC **A61M 16/0069** (2014.02); **A61M 16/024**
(2017.08); **A61M 2016/0015** (2013.01);
(Continued)

(57) **ABSTRACT**

A pressure control ventilation system (10) configured to provide airway release ventilation synchronous with a breathing subject that includes a pressure generator (12) configured to generate pressurized flow of breathable gas to a subject, one or more sensors (28) configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow, one or more processors (14) configured to execute computer modules comprising: a synchronization module (16) configured to detect inspiratory (39, 45) and expiratory (40, 44, 59) flow phases of the subject based at least on the signals; an interval module (18) configured to define time intervals (54, 60); a control module (20) configured to control the generator to deliver flow fluctuating between a first pressure range (48) to maintain adequate lung volume and a second pressure range (50) to facilitate CO₂ exhalation, the control including: delivering the flow in the first range at the beginning (56) of a first time interval (54); adjusting the flow from the first to the second range responsive to a detection of a start (42) of a first expiratory flow phase (40) in the first time interval; maintaining the flow at the second range over the first expiratory phase; and maintaining the flow at the first range

(Continued)



US 10,518,050 B2

Page 2

over a second expiratory phase (44) starting in the first time interval and following the first expiratory phase.

15 Claims, 4 Drawing Sheets

(52) **U.S. Cl.**

CPC A61M 2016/0039 (2013.01); A61M 2205/3365 (2013.01)

(58) **Field of Classification Search**

CPC A61M 16/0066; A61M 16/0069; A61M 16/022; A61M 16/024; A61M 2016/0015; A61M 2016/0018; A61M 2016/003; A61M 2016/0033; A61M 2016/0039; A61M 2205/3334; A61M 2205/3365

See application file for complete search history.

(56)

References Cited

U.S. PATENT DOCUMENTS

6,213,119 B1 * 4/2001 Brydon A61M 16/024
128/204.18

2003/0045807	A1 *	3/2003	Daniels, II	A61B 5/083 600/538
2003/0111078	A1 *	6/2003	Habashi	A61M 16/00 128/204.18
2006/0000475	A1 *	1/2006	Matthews	A61M 16/0051 128/204.21
2006/0011195	A1	1/2006	Zarychta	
2006/0124130	A1	6/2006	Bonassa	
2007/0215146	A1 *	9/2007	Douglas	A61M 16/00 128/200.24
2008/0295839	A1 *	12/2008	Habashi	A61M 16/0051 128/204.22
2008/0295840	A1	12/2008	Glaw	
2009/0095297	A1	4/2009	Hallett	
2011/0023880	A1	2/2011	Thiessen	
2011/0197887	A1 *	8/2011	Truschel	A61M 16/0051 128/204.23
2011/0240025	A1 *	10/2011	Mechlenburg	A61M 16/026 128/204.21
2012/0055484	A1	3/2012	Shaw	
2012/0234324	A1 *	9/2012	Orr	A61M 16/00 128/204.22

* cited by examiner

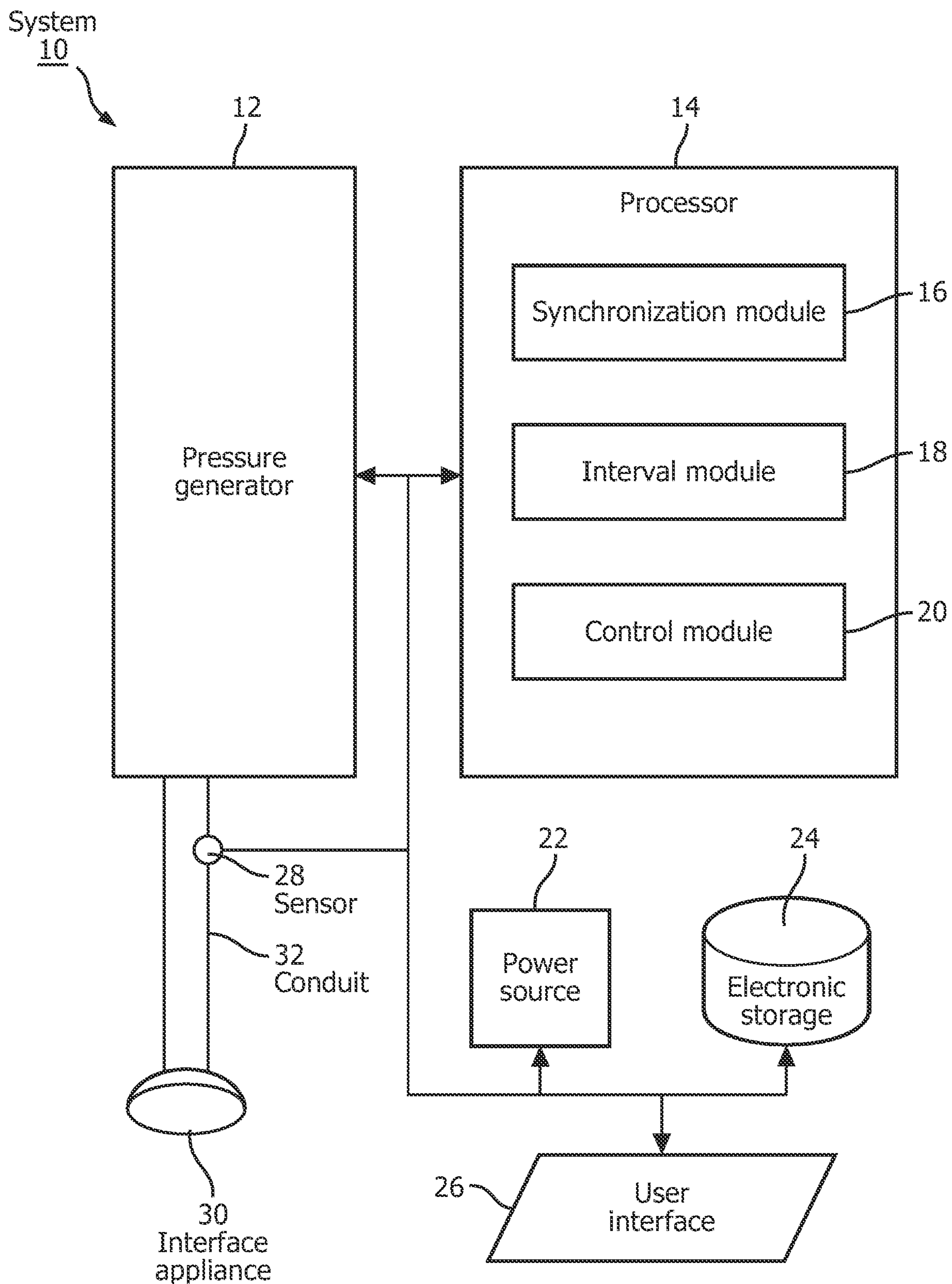


FIG. 1

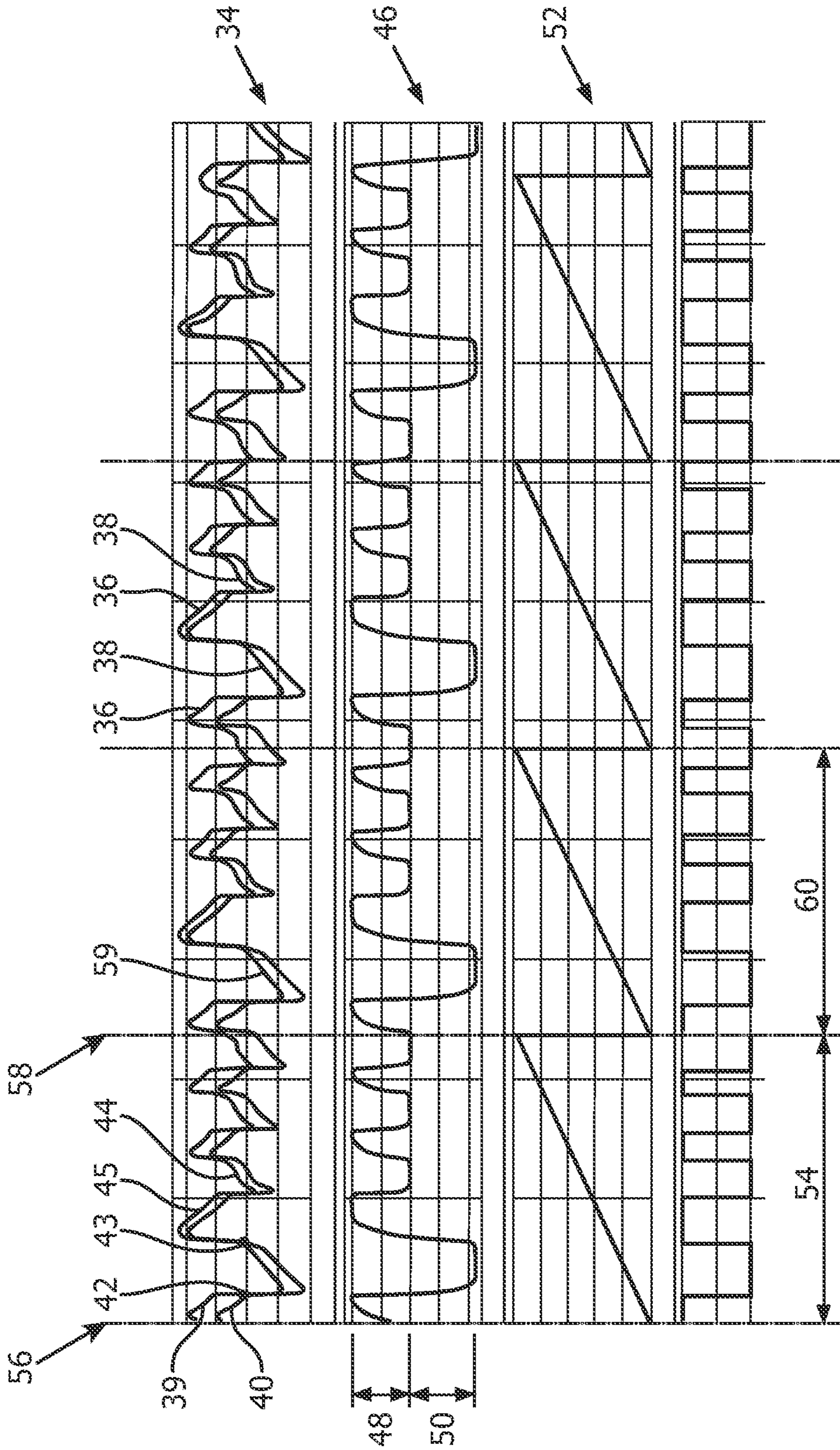


FIG. 2

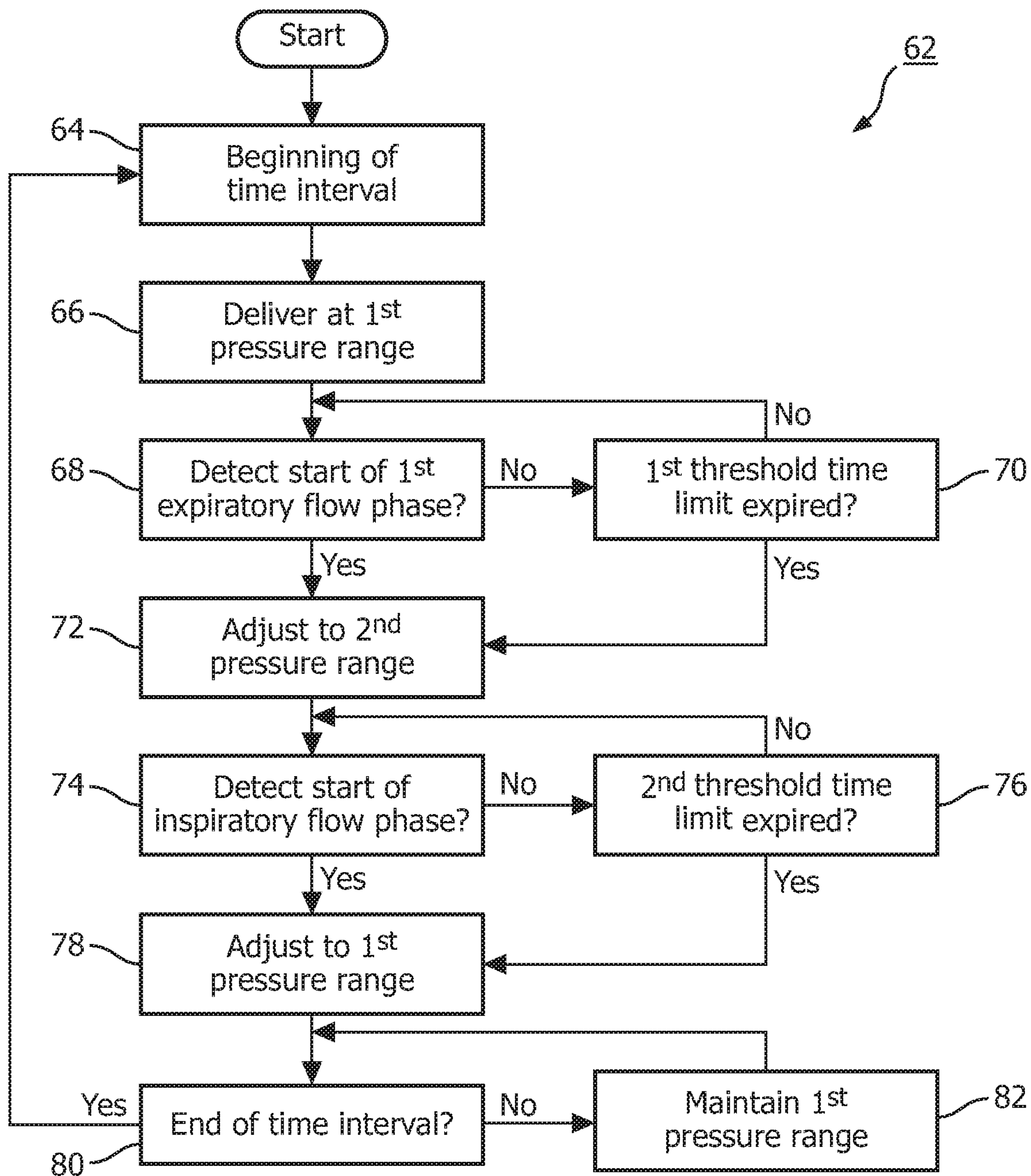


FIG. 3

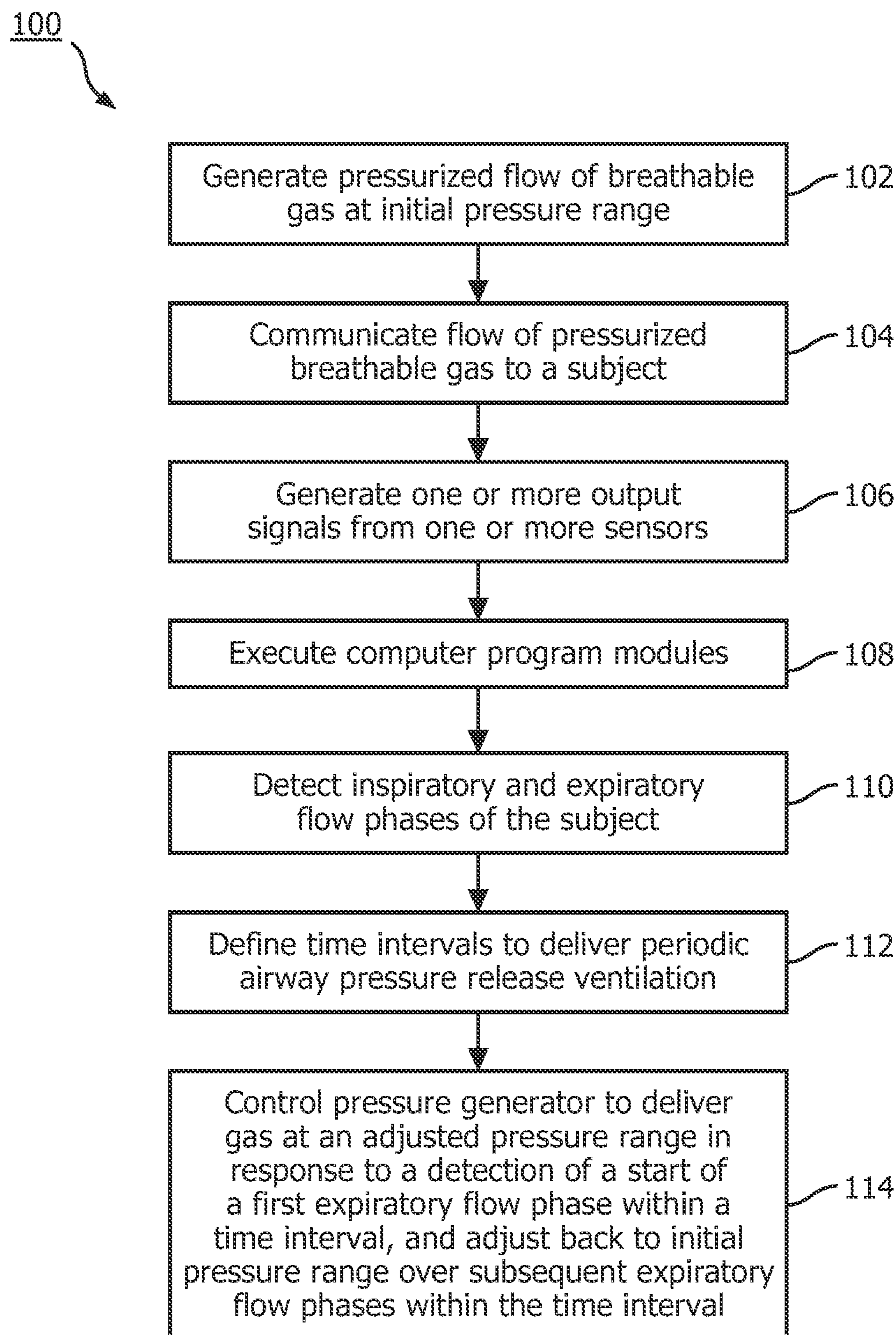


FIG. 4

SYNCHRONOUS AIRWAY PRESSURE RELEASE VENTILATION

This patent application claims the priority benefit under 35 U.S.C. § 371 of international patent application no. PCT/IB2014/061965, filed Jun. 5, 2014, which claims the priority benefit under 35 U.S.C. § 119(e) of U.S. Provisional Application No. 61/833,552 filed on Jun. 11, 2013, the contents of which are herein incorporated by reference.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present disclosure pertains to systems and methods for pressure control ventilation, and, in particular, to provide airway pressure release ventilation which is synchronous to a patient's breathing pattern.

2. Description of the Related Art

Airway pressure release ventilation is a method of bilevel pressure ventilation that produces a severe inverse ratio to periodically eliminate carbon dioxide from the airway of a subject, while maintaining a high positive airway pressure or Mean Airway Pressure for alveolar recruitment. It was described by Stocks and Downs in 1987 and is indicated to treat acute lung injury along with other respiratory complications.

SUMMARY OF THE INVENTION

Accordingly, one or more aspects of the present disclosure relate to a pressure control ventilation system configured to provide airway pressure release ventilation synchronous with a breathing subject, the pressure support system comprising a pressure generator configured to generate pressurized flow of breathable gas, one or more sensors configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas, and one or more processors configured to execute computer program modules.

The computer program modules comprise a synchronization module configured to detect inspiratory and expiratory flow phases of the breathing subject, including detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject, the detection based in part on the output signals of the one or more sensors, an interval module configured to define time intervals, the time intervals including beginning times and end times, and a control module configured to control the pressure generator to deliver pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges such that at the first higher pressure range the lungs of the subject are supported by the pressurized flow of breathable gas to maintain adequate lung volume, and at the second pressure range pressure through the airway of the subject is reduced to facilitate exhalation of carbon dioxide from the subjects lungs and facilitate tidal ventilation.

The control of the pressure generator includes, effectuating delivery of the pressurized flow of breathable gas to the airway of the subject with the first pressure range at the beginning time of a time interval, effectuating adjustment of the pressurized flow from the first pressure range to the second pressure range responsive to a detection by the synchronization module of a start of a first expiratory flow phase in the time interval or by a predetermined set time period, effectuating maintenance of delivery of the pressurized flow of breathable gas at the second pressure range over the expiratory flow phase; and effectuating maintenance of

delivery of the pressurized flow of breathable gas at the first pressure range responsive to a detection by the synchronization module of the start of inspiration or by a predetermined set time period following the first expiratory flow phase. Furthermore, the pressurized flow of breathable gas will be maintained at the first pressure range over all expiratory and inspiratory flows following the first expiratory flow phase until the end time of the time interval.

Yet another aspect of the present disclosure relates to a method for delivering pressure control ventilation configured to provide airway pressure release ventilation synchronous with a breathing subject that includes a pressure generator configured to generate pressurized flow of breathable gas to a subject, a conduit for communicating pressurized flow from the pressure generator to a subject, an interface appliance to communicate the pressurized flow to the airway of the subject, one or more sensors configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow, one or more processors configured to execute computer modules, a power source, a user interface, and electronic storage.

The method comprises generating the pressurized flow of breathable gas with the pressure generator, communicating the pressurized flow of breathable gas to the airway of the subject with the interface appliance, generating output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas with the one or more sensors, executing computer program modules on the processor, wherein the computer program module detect inspiratory and expiratory flow phases of the breathing subject including detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject, defining time intervals for providing periodic airway pressure release ventilation including defining beginning times and end times of the time intervals, and controlling the pressure generator to deliver pressurized flow of breathable gas with a pressure that fluctuates between pressure ranges.

Controlling the pressure generator includes controlling the pressure generator to deliver pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges such that at the first pressure range the lungs of the subject are supported by the pressurized flow of breathable gas to maintain adequate lung volume, and at the second pressure range the pressure through the airway of the subject is reduced to facilitate exhalation of carbon dioxide from the subjects lungs and encourage tidal ventilation, effectuating delivery of the pressurized flow of breathable gas to the airway of the subject with the first pressure range at the beginning time of a time interval, effectuating adjustment of the pressurized flow from the first pressure range to the second pressure range responsive to a detection of a start of a first expiratory flow phase in the time interval, effectuating maintenance of delivery of the pressurized flow of breathable gas at the second pressure range over the first expiratory flow phase, and effectuating maintenance of delivery of the pressurized flow of breathable gas at the first pressure range with the option of a programmable pressure support during the inspiratory flow phase following the first expiratory flow phase, and maintaining pressure at the first pressure range over all other expiratory flow phases following the first expiratory flow phase until the start of a new time interval.

Still another aspect of present disclosure relates to a pressure control ventilation system configured to provide airway pressure release ventilation synchronous with a breathing subject, the pressure support system comprising means for generating the pressurized flow of breathable gas,

means for communicating the pressurized flow of breathable gas to the airway of the subject, means for generating output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas, means for executing computer program modules, means for detecting inspiratory and expiratory flow phases of the breathing subject including detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject, means for defining time intervals for providing periodic airway pressure release ventilation including defining beginning times and end times of the time intervals, and means for controlling the pressure generator to deliver pressurized flow of breathable gas with a pressure that fluctuates between pressure ranges.

The means for controlling the pressure generator includes means for controlling the pressure generator to deliver pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges such that at the first pressure range the lungs of the subject are supported by the pressurized flow of breathable gas to maintain adequate lung volume, and at the second pressure range pressure through the airway of the subject is reduced to facilitate exhalation of carbon dioxide from the subjects lungs and encourage tidal ventilation, effectuating delivery of the pressurized flow of breathable gas to the airway of the subject with the first pressure range at the beginning time of a time interval, effectuating adjustment of the pressurized flow from the first pressure range to the second pressure range responsive to a detection of a start of a first expiratory flow phase in the time interval, effectuating maintenance of delivery of the pressurized flow of breathable gas at the second pressure range over the expiratory flow phase, and effectuating maintenance of delivery of the pressurized flow of breathable gas at the first pressure range over all other expiratory flow phases following the first expiratory flow phase until the end of the time interval.

These and other objects, features, and characteristics of the present disclosure, as well as the methods of operation and functions of the related elements of structure and the combination of parts and economies of manufacture, will become more apparent upon consideration of the following description and the appended claims with reference to the accompanying drawings, all of which form a part of this specification, wherein like reference numerals designate corresponding parts in the various figures. It is to be expressly understood, however, that the drawings are for the purpose of illustration and description only and are not intended as a definition of the limits of the disclosure.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a pressure control ventilation system providing airway pressure release ventilation which is synchronous to a patient's breathing pattern that includes a pressure generator configured to generate pressurized flow of breathable gas to a subject, a conduit for communicating pressurized flow from the pressure generator to a subject, an interface appliance to communicate the pressurized flow to the airway of the subject, one or more sensors configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow, one or more processors configured to execute computer modules, a power source, a user interface, and electronic storage;

FIG. 2 is an illustration of gas parameters measured over time relating to output signals of the sensors of the pressure control ventilation system;

FIG. 3 is a method for controlling the pressure generator of the pressure control ventilation system; and

FIG. 4 is a method for delivering pressure control ventilation which provides periodic airway pressure release ventilation which is synchronous to a patient's breathing pattern.

As used herein, the singular form of "a", "an", and "the" include plural references unless the context clearly dictates otherwise. As used herein, the statement that two or more parts or components are "coupled" shall mean that the parts are joined or operate together either directly or indirectly, i.e., through one or more intermediate parts or components, so long as a link occurs. As used herein, "directly coupled" means that two elements are directly in contact with each other. As used herein, "fixedly coupled" or "fixed" means that two components are coupled so as to move as one while maintaining a constant orientation relative to each other.

As used herein, the word "unitary" means a component is created as a single piece or unit. That is, a component that includes pieces that are created separately and then coupled together as a unit is not a "unitary" component or body. As employed herein, the statement that two or more parts or components "engage" one another shall mean that the parts exert a force against one another either directly or through one or more intermediate parts or components. As employed herein, the term "number" shall mean one or an integer greater than one (i.e., a plurality).

Directional phrases used herein, such as, for example and without limitation, top, bottom, left, right, upper, lower, front, back, and derivatives thereof, relate to the orientation of the elements shown in the drawings and are not limiting upon the claims unless expressly recited therein.

FIG. 1 schematically illustrates an exemplary embodiment of a pressure control ventilation system 10 configured to provide periodic airway pressure release ventilation synchronous to a subject's breathing pattern. Pressure control ventilation system 10 may be configured to provide the pressure support and ventilation in the form of a pressurized flow of breathable gas that is delivered to the airway of the subject. Pressure control ventilation system 10 may be configured to deliver pressurized flow of breathable gas in multiple pressure ranges. Pressure control ventilation system 10 may be configured to allow subjects to breathe spontaneously during delivery of the pressurized flow of breathable gas at a first pressure range. Pressure control ventilation system 10 may be configured to provide pressure release in the form of delivery of pressurized flow of breathable gas at a second pressure range, wherein the second pressure range is lower than the first pressure range.

The pressure release provided by delivery of pressurized flow of breathable gas at the second pressure range may facilitate the exhalation of carbon dioxide from the subjects' airway at periodic intervals, while delivery of pressurized flow of breathable gas at the first pressure range may improve oxygenation through greater alveolar recruitment. The pressure level being delivered within the first pressure range may be varied to a relatively higher pressure level to provide additional pressure support in the first pressure range during inspiratory flow phases. The pressure level being delivered within the first pressure range may be varied to a relatively lower pressure level to provide pressure relief in the first pressure range during expiratory flow phases.

The present disclosure contemplates that pressure control ventilation system 10 may be used to treat symptoms and/or conditions related to Acute Respiratory Distress Syndrome, Acute Lung Injury, and other forms of respiratory failure or insufficiency, and/or other uses. The other uses may include

treatment of central or obstructive sleep apnea, Obesity Hypoventilation Syndrome and related forms of chronic hypoventilation, and/or other uses.

In some embodiments, pressure control ventilation system **10** comprises one or more of a pressure generator **12**, one or more processors **14**, a power source **22**, electronic storage **24**, a user interface **26**, one or more sensors **28**, and/or other components.

Pressure generator **12** is configured to generate a pressurized flow of breathable gas for delivery to the airway of a subject. Pressure generator **12** may include a conduit **32** providing a flow path for delivering the breathable gas to the subject. Conduit **32** may comprise one or more of a flexible conduit, sealed tubing, and/or other component suitable for delivery of pressurized breathable gas. Conduit **32** may be integrally connected to an interface appliance **30**. Interface appliance **30** may comprise one or more of a nasal mask, nasal cannula, a full face mask, a nasal pillow mask, a hybrid mask, an oral mask, a total face mask, an endotracheal tube, and/or other invasive and/or non-invasive interface appliance configured to communicate a flow of gas to the airway of a subject. In some embodiments, interface appliance **30** may be removably coupled to conduit **32**. Interface appliance **30** may be removed for cleaning and/or for other purposes.

Pressure generator **12** generates pressurized flow of breathable gas according to one or more parameters of the flow of gas (e.g., flow rate, pressure, volume, temperature, gas composition, etc.) for therapeutic purposes, and/or for other purposes. By way of a non-limiting example, pressure generator **12** may be configured to generate pressurized flow at a flow rate and/or pressure of the flow of gas to provide pressure support and/or pressure release ventilation to the airway of a subject.

Pressure generator **12** may receive a flow of gas from a gas source, such as the ambient atmosphere, and elevates the pressure of that gas for delivery to the airway of a subject at a pressurized flow. In some embodiments, pressure generator **12** may receive a flow of gas from a gas source through an inlet port (not shown). Pressure generator **12** may be any device, such as, for example, a pump, blower, piston, or bellows, that is capable of elevating the pressure of the received gas for delivery to a subject. Pressure generator **12** may comprise one or more valves for adjusting the delivery of the pressure/flow of gas. The present disclosure also contemplates controlling the operating speed of the blower, either alone or in combination with such valves, to control the pressure/flow of gas provided to the subject.

In some embodiments, pressure generator **12** is configured to supply a pressurized flow of breathable gas at a first pressure range of about 0 to 50 cm H₂O. In some embodiments, pressure generator **12** may be configured to supply a pressurized flow of breathable gas at a second pressure range of about 0 to 30 cm H₂O. In some embodiments, pressure generator **14** may be configured to supply a pressurized flow of breathable gas at other pressures and/or pressure ranges.

One or more sensors **28** are configured to generate output signals conveying information related to one or more parameters of the gas within pressure control ventilation system **10**. The one or more parameters of the gas within pressure control ventilation system **10** may comprise gas parameters related to the pressurized flow of breathable gas generated by pressure generator **12**, breathing parameters related to respiration of the subject employing pressure control ventilation system **10**, and/or other parameters. Sensors **28** may comprise one or more sensors that measure such parameters directly (e.g., through fluid communication with the flow of

gas in interface appliance **30**, and/or conduit **32**). Sensors **28** may comprise one or more sensors that generate surrogate output signals related to the one or more parameters indirectly. For example, sensors **28** may comprise one or more sensors configured to generate an output based on an operating parameter of pressure generator **12** (e.g., patient flow and/or pressure estimations from motor current, voltage, rotational velocity, and/or other operating parameters), and/or other sensors.

The one or more gas parameters of the pressurized flow of breathable gas may comprise, for example, one or more of a flow rate, a volume, a pressure, humidity, temperature, acceleration, velocity, and/or other gas parameters. Breathing parameters related to the respiration of a subject may comprise a tidal volume, respiratory flow phase (e.g., inspiratory flow phases, expiratory flow phases, etc.), a timing (e.g., start and/or end of inspiratory flow phases, start and/or end of expiratory flow phases, etc.), a respiration rate, a duration (e.g., of inspiratory flow phases, of expiratory flow phases, of a single breathing cycle, etc.), respiration frequency, and/or other breathing parameters.

Although sensors **28** are illustrated at a single location in pressure control ventilation system **10**, this is not intended to be limiting. Sensors **28** may comprise sensors disposed in a plurality of locations, such as for example, at various locations within (or in communication with) conduit **32**, within pressure generator **12**, within (or in communication with) interface appliance **30**, and/or other locations.

Processor **14** is configured to provide information processing capabilities in pressure control ventilation system **10**. As such, processor **14** may comprise one or more of a digital processor, an analog processor, a digital circuit designed to process information, an analog circuit designed to process information, a state machine, and/or other mechanisms for electronically processing information. Although processor **14** is shown in FIG. **1** as a single entity, this is for illustrative purposes only. In some implementations, processor **14** may comprise a plurality of processing units. These processing units may be physically located within the same device (e.g., pressure generator **12**), or processor **14** may represent processing functionality of a plurality of devices operating in coordination.

As shown in FIG. **1**, processor **14** is configured to execute one or more computer program modules. The one or more computer program modules may comprise one or more of a synchronization module **16**, an interval module **18**, a control module **20**, and/or other modules. Processor **14** may be configured to execute modules **16**, **18**, and/or **20** by software; hardware; firmware; some combination of software, hardware, and/or firmware; and/or other mechanisms for configuring processing capabilities on processor **14**.

It should be appreciated that although modules **16**, **18**, and **20** are illustrated in FIG. **1** as being co-located within a single processing unit, in implementations in which processor **14** comprises multiple processing units, one or more of modules **16**, **18**, and/or **20** may be located remotely from the other modules. The description of the functionality provided by the different modules **16**, **18**, and/or **20** described below is for illustrative purposes, and is not intended to be limiting, as any of modules **16**, **18**, and/or **20** may provide more or less functionality than is described. For example, one or more of modules **16**, **18**, and/or **20** may be eliminated, and some or all of its functionality may be provided by other modules **16**, **18**, and/or **20**. As another example, processor **14** may be configured to execute one or more additional modules that may perform some or all of the functionality attributed below to one of modules **16**, **18**, and/or **20**.

Synchronization module **16** is configured to detect inspiratory and expiratory flow phases of the respiration cycles of a breathing subject employing pressure control ventilation system **10**. The detection may be based on the one or more output signals from the one or more sensors **28** conveying information related to flow rate parameters of the gas within pressure control ventilation system **10**.

By way of illustrations, FIG. **2** illustrates plots of gas parameters of the pressurized flow of breathable gas over time (e.g., represented by output signals of one or more sensors). Plot **34** provides a graphical representation of flow rate. In plot **34**, the changing respiratory flow rate of the pressurized flow of breathable gas illustrates inspiratory flow phases (e.g., peaks **36** representing inhalation) when flow is positive relative to zero or baseline, and troughs **38** which represent expiratory flow phases (e.g., exhalation) when flow is negative relative to zero or baseline. Transitions between inspiratory flow phases and expiratory flow phases may be determined by the transition or an anticipated transition based on flow trajectory between troughs **38** and peaks **36** as shown graphically in plot **34**. Plot **46** provides a graphical representation of the pressure of the pressurized flow of breathable gas generated by pressure generator **12** (e.g., represented by output signals of one or more sensors).

Returning to FIG. **1**, synchronization module **16** is configured to detect starts and ends of inspiratory flow phases (e.g., peaks **36** as shown in FIG. **2**) and expiratory flow phases (e.g., troughs **38** as shown in FIG. **2**). For example, in FIG. **2**, a first expiratory flow phase **40** is shown in plot **34**. First expiratory flow phase **40** includes a start **42** which occurs at the transition between a first inspiratory flow phase **39** (e.g., temporally first flow phase within the time interval and immediately preceding the first expiratory flow phase **40**) and the first expiratory flow phase **40**.

In plot **34**, the end of the first expiratory flow phase **40** may be indicated by a start **43** of a second inspiratory flow phase **45** immediately following the first expiratory flow phase **40**. The start **43** of second inspiratory flow phase **45** indicates the end of first expiratory flow phase **40**. In addition, a second expiratory flow phase **44** may also be indicated as the trough immediately following second inspiratory flow phase **45**. Second expiratory flow phase **44**, does not produce and airway release as during first expiratory phase **40**, because interval **54** has yet to expire.

It is noted that although detailed descriptions of start **42** of first expiratory flow phase **40** and start **43** of second inspiratory flow phase **45** are provided, it is to be understood that starts and ends of any and all inspiratory and expiratory flow phases of a respiration cycle of a breathing subject, including those not shown directly in FIG. **2**, can be determined from plot **34**. As such it is to be understood that detection of starts and ends may be carried out longer or shorter than the time periods depicted by the plots shown in FIG. **2**.

It is to be understood for convention in this disclosure, that transitions between inspiratory flow phases (e.g., peaks **36**) and expiratory flow phases (e.g., troughs **38**) includes both the flow rate measurements representing the end of the inspiratory flow phase and the start of the expiratory flow phase. Therefor the term “end of the inspiratory flow phase” essentially refers to the same flow rate measurements as the term “start of the expiratory flow phase” which immediately follows the inspiratory flow phase. Further it is to be understood that transitions between expiratory flow phases (e.g., troughs **38**) and inspiratory flow phases (e.g., peaks **36**) includes both the flow rate measurement representing the end of the expiratory flow phase and the start of the

inspiratory flow phase. Therefor the term “end of the expiratory flow phase” refers generally to the same flow rate measurements as the term “start of the inspiratory flow phase” which immediately follows the expiratory flow phase.

Returning to FIG. **1**, interval module **18** is configured to define time intervals for which pressure control ventilation system **10** provides periodic airway pressure release ventilation. Individual time intervals may encompass one occurrence of airway pressure release ventilation. Individual time intervals may encompass more than one occurrence of airway pressure release ventilation. Time intervals may include beginning times and end times. Time intervals may be defined by user selection through user interface **26** of pressure control ventilation system **10**. The user may be the subject, a health care professional, and/or other user. Time intervals may be predetermined by pressure control ventilation system **10**. For example time intervals can be set to 15 seconds (or other amount). Time intervals may be dynamically defined by the particular breathing patterns of a subject. For example, intervals may be defined by the average amount of time it takes for a subject to complete four (or other amount) of inspiratory and expiratory flow phases (e.g., breaths).

By way of illustrations, FIG. **2** illustrates plot **52** providing a graphical representation of time intervals. Plot **52** depicts a first time interval **54**, a second time interval **60**, and/or more and/or less time intervals in which periodic airway pressure release ventilation is provided. In plot **52**, the beginning **56** and end **58** of first time interval **54** are temporally indicated. The end **58** of first time interval **54** is defined as the start of second time interval **60**.

Flow phases (e.g., peaks **36** and troughs **38** in plot **34**) may be temporally defined with respect to time intervals. Flow phases may be designated as temporally first, second, third, etc., flow phases with respect to the beginning and end times of the time intervals. For example, in plot **34** of FIG. **2**, first expiratory flow phase **40** is the temporally first expiratory flow phase within first time interval **54** with respect to beginning time **56**. Second expiratory flow phase **44** is the temporally second expiratory flow phase with respect to first time interval **54**, and so forth. Subsequent expiratory flow phases following first expiratory flow phase **40** may be designated as temporally first expiratory flow phases due to the relationship of the start of a particular expiratory flow phase (e.g., transition from peak **36** to trough **38**) with respect a start of a time interval. For example, fifth expiratory flow phase **59** (e.g., the fifth trough **38** when counting left to right) is the temporally first expiratory flow phase with respect to second time interval **60**.

In FIG. **1**, control module **20** is configured to effectuate delivery and/or adjustment and/or maintenance of a pressure and/or pressure range of pressurized flow of breathable air generated by pressure generator **14** in a variety of ways. Control module **20** is configured to control pressure generator **12** to deliver pressurized flow of breathable gas with a pressure that fluctuates between particular pressure levels and/or pressure ranges. Control module **20** may be configured to effectuate delivery of the pressurized flow of breathable gas to the airway of the subject at an initial pressure level and/or pressure range at the beginning of the time intervals (e.g., at the beginning times or toward the beginning).

Control module **20** may be configured to effectuate adjustment of the pressurized flow from the initial pressure and/or or pressure range to an adjusted pressure and/or pressure range responsive to a detection by synchronization module

16 of a start of a temporally first (and/or second, third, fourth, etc.) expiratory flow phase within the time intervals, and/or other detection by synchronization module 16. Control module 20 may be configured to effectuate maintenance of delivery of the pressurized flow of breathable gas at the adjusted pressure and/or pressure range over the duration of the temporally first (and/or second, third, fourth, etc.) expiratory flow phase, and/or other time duration.

Control module 20 may be configured to effectuate adjustment of the pressurized flow from the adjusted pressure and/or pressure range back to the initial pressure level and/or pressure range, and/or other pressure level and/or pressure range, after the expiration of the duration of the temporally first (and/or second, third, fourth, etc.) expiratory flow phase, and/or other time duration. Control module 20 may be configured to effectuate maintenance of delivery of the pressurized flow of breathable gas at the initial pressure and/or pressure range, and/or other pressure and/or pressure range, over subsequent expiratory flow phases following the temporally first (and/or second, third, fourth, etc.) expiratory flow phase at least until the expiration of the time interval.

Control module 20 is configured to control pressure generator 12 to deliver pressurized flow of breathable gas at a first pressure range (e.g., first pressure range 48 in plot 46 of FIG. 2). Delivery of the pressurized flow of breathable gas allows subjects to breathe spontaneously. At the first pressure range, the lungs of the subject are supported by the pressurized flow of breathable gas to maintain adequate lung volume. Delivery of pressurized flow of breathable gas by pressure generator 12 at the first pressure range may improve oxygenation through greater alveolar recruitment.

Control module 20 is configured to control pressure generator 12 to deliver pressurized flow of breathable gas at a second pressure range (e.g., second pressure range 50 shown in plot 46 of FIG. 2) which facilitates periodic exhalation of carbon dioxide from the subjects' airway at periodic intervals. The second pressure range may be lower than first pressure range. At the second pressure range, pressure of the pressurized flow generated by pressure generator 12 through the airway of the subject is reduced to facilitate exhalation of carbon dioxide from the subject's lungs. The frequency at which control module 20 effectuates delivery of pressurized flow of breathable gas at the second pressure range may be based on detections of any one of temporally first, second, third, fourth, etc. expiratory flow phase within the time intervals.

By way of illustration, FIG. 3 depicts exemplary, non-limiting method 62 showing operations of control module 20 of FIG. 1 in controlling pressure generator 12 of FIG. 1 to deliver the pressurized flow of breathable gas so that pressure fluctuates between the first pressure range and the second pressure range. Operations 64 and 66 perform effectuating delivery of the pressurized flow of breathable gas to the airway of the subject at an initial pressure and/or pressure range at the beginning times of the time intervals. Operations 68 and 72 perform adjustment of the pressurized flow from an initial pressure and/or pressure range to an adjusted pressure and/or pressure range responsive to a detection (e.g., by synchronization module 16 of FIG. 1) of a start of a temporally first (and/or second, third, fourth etc.) expiratory flow phase within the time intervals, and/or other detection. Absent a detection of the start of a temporally first (and/or second, third, fourth etc.) expiratory flow phase within time intervals, at operation 70, adjustment of the pressurized flow from the initial pressure and/or pressure range to the adjusted pressure and/or pressure range is

performed responsive to a detection of an expiration of a first threshold time limit following the beginning of the time interval.

By way of further illustration, returning to FIG. 2, plot 46 depicts the delivery of the pressurized flow of breathable gas to the airway of the subject at first pressure range 48 at the beginning time 56 of first time interval 54. Adjustment of the pressurized flow from the first pressure range 48 to the second pressure range 50 is depicted responsive to a detection of start 42 of first expiratory flow phase 40 in the first time interval 54 (the first expiratory flow phase 40 being the temporally first expiratory flow phase in first time interval 54). Absent a detection (e.g., by synchronization module 16 of FIG. 1) of start 42 of first expiratory flow phase 40 (e.g., temporally first expiratory flow phase within first time interval 54), adjustment of the pressurized flow from the first pressure range 48 to the second pressure range 50 is responsive to a detection of an expiration of a first threshold time limit following beginning 56 of first time interval 54.

First threshold time limit may be defined by user selection (e.g., through user interface 26 of pressure control ventilation system 10 in FIG. 1). The user may be the subject, a health care professional, and/or other user. First threshold time limit may be predetermined. For example threshold time limit may be set to 2 seconds (or other amount). First threshold time limit may be dynamically defined by the particular breathing patterns of a subject. For example, first threshold time limit may be defined by the average amount of time it takes for the subject to complete inspiratory flow phases (e.g., inhalations).

Returning to FIG. 3, at an operation 74, maintenance of delivery of the pressurized flow of breathable gas at the adjusted pressure level and/or pressure range is performed over the duration of the temporally first (and/or second, third, fourth etc.) expiratory flow phase, and/or other time duration. The duration of the temporally first (and/or second, third, fourth etc.) expiratory flow phase may be the time between a detection of the start of the temporally first (and/or second, third, fourth etc.) expiratory flow phase and the start of the inspiratory flow phase immediately following the temporally first (and/or second, third, fourth, etc.) expiratory flow phase within the time interval.

Absent a detection of the start of the inspiratory flow phase immediately following the temporally first (and/or second, third, fourth etc.) expiratory flow phase within the time interval, an operation 76 may perform maintenance of the delivery of the pressurized flow of breathable gas at the adjusted pressure and/or range over a duration of time which is the time between the start of the temporally first (and/or second, third, fourth etc.) expiratory phase and the end of a second threshold time limit following the start of the temporally first (and/or second, third, fourth etc.) expiratory flow phase. At an operation 78 adjustment of the pressurized flow from the adjusted pressure and/or pressure range back to the initial pressure and/or pressure range, and/or other pressure and/or pressure range is performed after the expiration of the duration of the temporally first (and/or second, third, fourth etc.) expiratory flow phase and/or other time duration associated with maintenance of delivery of the pressurized flow of breathable gas at the adjusted pressure and/or pressure range.

For example returning to FIG. 2, maintaining the delivery of the pressurized flow of breathable gas at the second pressure range 50 over the first expiratory flow phase 40 (e.g., temporally first expiratory flow phase within first interval 54) includes maintaining the delivery of the pressurized flow of breathable gas during the time between the

11

start **42** of the first expiratory flow phase **40** and start **43** of second inspiratory flow phase **45** (e.g., the inspiratory flow phase immediately following first expiratory flow phase **40**). Absent a detection of the start **43** of second inspiratory flow phase **45**, maintenance of delivery of pressurized flow of breathable gas at second pressure range **50** may be performed during the time between the start **42** of the first expiratory flow phase **40** and the end of a second threshold time limit following the start **42** of the first expiratory flow phase **40**. Second threshold time limit may be defined by user selection.

The user may be the subject, a health care professional, and/or other user. Second threshold time limit may be predetermined. For example threshold time limit may be set to 3 seconds (or other amount). Second threshold time limit may be dynamically defined by the particular breathing patterns of a subject. For example, second threshold time limit may be defined by the average amount of time it takes for the subject to complete expiratory flow phases (e.g., exhalations). Responsive to the detection of the expiration of the first expiratory flow phase **40** (e.g., detection of the start **43** of second inspiratory flow phase **45**), and/or detection of the expiration of the second threshold time limit following the start **42** of first expiratory flow phase **40**, adjustment of pressurized flow from second pressure range **50** back to first pressure range **48** is performed.

Returning to FIG. 3, at operations **80** and **82**, maintenance of delivery of the pressurized flow of breathable gas at the initial pressure level and/or pressure range, and/or other pressure level and/or pressure range, over subsequent expiratory and inspiratory flow phases following the temporally first (and/or second, third, fourth etc.) expiratory flow phase is performed at least until the expiration of the time interval. For example, returning to FIG. 2, maintenance of delivery of the pressurized flow of breathable gas first pressure range **48** over subsequent expiratory and inspiratory flow phases following the first expiratory flow phase **40** of first time interval **54** is performed at least until the end **58** of first time interval **54**. Maintaining the delivery within first pressure level **48** may include, for example, that the pressure level being delivered within first pressure range **48** may be varied to a relatively higher pressure level within first pressure range **48** to provide additional pressure support during inspiratory flow phases following first expiratory flow phase **40**. The pressure level being delivered within first pressure range **48** may be varied to a relatively lower pressure level to provide pressure relief in the first pressure range **48** during expiratory flow phases following first expiratory flow phase **40**.

FIG. 4 illustrates a method **100** of delivering pressure control ventilation configured to provide periodic airway pressure release ventilation synchronous to a subject's breathing pattern. The delivery of pressure control ventilation may include a pressure generator configured to generate pressurized flow of breathable gas to a subject, a conduit for communicating pressurized flow from the pressure generator to a subject, an interface appliance to communicate the pressurized flow to the airway of the subject, one or more sensors configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow, one or more processors configured to execute computer modules, a power source, a user interface, electronic storage, and/or other components. The operations of method **100** presented below are intended to be illustrative. In some embodiments, method **100** may be accomplished with one or more additional operations not described, and/or without one or more of the operations

12

discussed. Additionally, the order in which the operations of method **100** are illustrated in FIG. 4 and described below is not intended to be limiting.

In some embodiments, method **100** may be implemented in one or more processing devices (e.g., a digital processor, an analog processor, a digital circuit designed to process information, an analog circuit designed to process information, a state machine, and/or other mechanisms for electronically processing information). The one or more processing devices may include one or more devices executing some or all of the operations of method **100** in response to instructions stored electronically on an electronic storage medium. The one or more processing devices may include one or more devices configured through hardware, firmware, and/or software to be specifically designed for execution of one or more of the operations of method **100**.

At an operation **102**, the pressurized flow of breathable gas is generated with the pressure generator. In some embodiments, operation **102** is performed by a pressure generator the same as or similar to pressure generator **12** (shown in FIG. 1 and described herein).

At an operation **104**, the pressurized flow of breathable gas is communicated to the airway of the subject with the interface appliance. In some embodiments, operation **104** is performed by an interface appliance the same as or similar to interface appliance **30** (shown in FIG. 1 and described herein).

At an operation **106**, one or more output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas are generated with the one or more sensors. In some embodiments, operation **106** is performed by sensors the same as or similar to sensors **28** (shown in FIG. 1 and described herein).

At an operation **108**, one or more program modules are executed by one or more processors. In some embodiments, operation **108** is performed by one or more processors the same as or similar to processor **14** (shown in FIG. 1 and described herein).

At an operation **110**, inspiratory and expiratory flow phases of the breathing subject are detected. The detection may include detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject. The detection may be based in part on the output signals of the one or more sensors from operation **106**. In some embodiments, operation **110** is performed by a synchronization module the same as or similar to synchronization module **16** (shown in FIG. 1 and described herein).

At an operation **112**, time intervals for providing periodic airway pressure release ventilation are defined. The time intervals may include beginning times and end times. In some embodiments, operation **112** is performed by an interval module the same as or similar to interval module **18** (shown in FIG. 1 and described herein).

At an operation **114**, the pressure generator is controlled to deliver pressurized flow of breathable gas with a pressure that fluctuates between pressure ranges. Such control may include controlling the pressure generator to deliver pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges such that at the first pressure range the lungs of the subject are supported by the pressurized flow of breathable gas to prevent collapse of the lungs, and at the second pressure range pressure through the airway of the subject is reduced to facilitate exhalation of carbon dioxide from the subjects lungs. Such control may include, effectuating delivery of the pressurized flow of breathable gas to the airway of the subject with the first pressure range at the beginning time of a first time interval,

effectuating adjustment of the pressurized flow from the first pressure range to the second pressure range responsive to a detection by the synchronization module of a start of a temporally first (and/or second, third, fourth, etc.) expiratory flow phase in the first time interval, effectuating maintenance of delivery of the pressurized flow of breathable gas at the second pressure range over the first (and/or second, third, fourth, etc.) expiratory flow phase, and effectuating maintenance of delivery of the pressurized flow of breathable gas at the first pressure range over subsequent expiratory flow phases following the first (and/or second, third, fourth, etc.) expiratory flow phase, that start in the first time interval. In some embodiments, operation 114 is performed by a control module the same as or similar to control module 20 (shown in FIG. 1 and described herein).

In the claims, any reference signs placed between parentheses shall not be construed as limiting the claim. The word “comprising” or “including” does not exclude the presence of elements or steps other than those listed in a claim. In a device claim enumerating several means, several of these means may be embodied by one and the same item of hardware. The word “a” or “an” preceding an element does not exclude the presence of a plurality of such elements. In any device claim enumerating several means, several of these means may be embodied by one and the same item of hardware. The mere fact that certain elements are recited in mutually different dependent claims does not indicate that these elements cannot be used in combination.

Although the description provided above provides detail for the purpose of illustration based on what is currently considered to be the most practical and preferred embodiments, it is to be understood that such detail is solely for that purpose and that the disclosure is not limited to the expressly disclosed embodiments, but, on the contrary, is intended to cover modifications and equivalent arrangements that are within the spirit and scope of the appended claims. For example, it is to be understood that the present disclosure contemplates that, to the extent possible, one or more features of any embodiment can be combined with one or more features of any other embodiment.

What is claimed is:

1. A pressure control ventilation system configured to provide airway pressure release ventilation synchronous with a breathing subject, the pressure support system comprising:

- (a) a pressure generator configured to generate a pressurized flow of breathable gas;
- (b) one or more sensors configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas; and
- (c) one or more processors configured to execute computer program modules, the computer program modules comprising:
 - (1) a synchronization module configured to detect inspiratory and expiratory flow phases of the breathing subject, including detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject, the detection based in part on the output signals of the one or more sensors;
 - (2) an interval module configured to:
 - (i) determine amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases, the amounts of time determined during ventilation based in part on the output signals of the one or more sensors; and

- (ii) define time intervals, the time intervals having start times and end times, the time intervals being determined based on the amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases during ventilation, the time intervals including a first time interval; and
- (3) a control module configured to control the pressure generator to deliver the pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges, the first pressure range being higher than the second pressure range, such that delivering the pressurized flow of breathable gas at the second pressure range reduces a gas pressure in the airway of the subject relative to the gas pressure when delivering the pressurized flow of breathable gas at the first pressure range, wherein such control of the pressure generator includes:
- (i) providing the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval, wherein the first time interval spans a plurality of respiratory cycles, and
 - (ii) providing the flow of breathable gas to the airway of the subject at the second pressure range responsive to the following conditions being detected:
 - (a) the first time interval has elapsed, and
 - (b) the synchronization module has detected a start of an expiratory flow phase.

2. The system of claim 1, wherein the control module is further configured to provide the flow of breathable gas to the airway of the subject at the first pressure range responsive to the synchronization module detecting an end of the expiratory flow phase.

3. The system of claim 1, wherein the control module is further configured such that providing the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval includes adjusting the pressure level of the pressurized flow to different values within the first pressure range during different expiratory flow phases during the first time interval.

4. The system of claim 1, wherein the control module is further configured such that providing the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval includes varying the pressure level of the pressurized flow within the first pressure range to a relatively higher pressure during inspiratory flow phases and to a relatively lower pressure during expiratory flow phases.

5. The system of claim 1, wherein the interval module is configured such that determining the amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases comprises determining the average amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases, and the time intervals are determined based on the average amounts of time.

6. A method for controlling a pressure generator to provide airway pressure release ventilation synchronous with a breathing subject, the method being implemented by a ventilation system including the pressure generator, one or more sensors configured to generate output signals conveying information related to one or more gas parameters of a pressurized flow generated by the pressure generator, one or more physical processors configured to execute computer program modules, a power source, a user interface, and electronic storage, the method comprising:

- generating the pressurized flow of breathable gas with the pressure generator;

15

generating output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas with the one or more sensors;

executing computer program modules on the processor;
 detecting inspiratory and expiratory flow phases of the breathing subject including detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject;

defining time intervals for providing periodic airway pressure release ventilation, the defining time intervals including:

determining amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases, the amounts of time determined during ventilation based in part on the output signals of the one or more sensors; and

defining beginning times and end times of the time intervals, the time intervals being determined based on the amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases during ventilation, the time intervals including a first time interval; and

controlling the pressure generator to deliver the pressurized flow of breathable gas with a pressure that fluctuates between pressure ranges, including controlling the pressure generator to deliver the pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges, the first pressure range being higher than the second pressure range, such that delivering the pressurized flow of breathable gas at the second pressure range reduces a gas pressure in the airway of the subject relative to delivering the pressurized flow of breathable gas at the first pressure range, wherein controlling the pressure generator comprises:

- i) providing the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval, wherein the first time interval spans a plurality of respiratory cycles, and
- ii) providing the flow of breathable gas to the airway of the subject at the second pressure range responsive to the following conditions being detected:
 - (a) the first time interval has elapsed, and
 - (b) a start of an expiratory flow phase has been detected.

7. The method of claim 6, wherein controlling the pressure generator to provide the flow of breathable gas to the airway of the subject at the first pressure range is responsive to detecting an end of the expiratory flow phase.

8. The method of claim 6, wherein providing the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval includes adjusting the flow of breathable gas to different values within the first pressure range during different expiratory flow phases during the first time interval.

9. The method of claim 6, wherein providing the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval includes varying the pressure level of the pressurized flow within the first pressure range to a relatively higher pressure during inspiratory flow phases and to a relatively lower pressure during expiratory flow phases.

10. The method of claim 6, determining the amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases comprises determining the average amounts of time the subject takes to complete inspira-

16

tory flow phases and expiratory flow phases, and the time intervals are determined based on the average amounts of time.

11. A pressure control ventilation system configured to provide airway pressure release ventilation synchronous with a breathing subject, the pressure support system comprising:

means for generating a pressurized flow of breathable gas;
 means for communicating the pressurized flow of breathable gas to the airway of the subject;
 means for generating output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas;

means for executing computer program modules;
 means for detecting inspiratory and expiratory flow phases of the breathing subject including detecting starts and ends of the inspiratory and expiratory flow phases of the breathing subject;

means for defining time intervals for providing periodic airway pressure release ventilation, defining time intervals including:

determining amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases, the amounts of time determined during ventilation based in part on the output signals of the one or more sensors; and

defining start times and end times of the time intervals, the time intervals being determined based on the amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases during ventilation, the time intervals including a first time; and

means for controlling the means for generating the pressurized flow of breathable gas to deliver the pressurized flow of breathable gas with a pressure that fluctuates between pressure ranges, the means for controlling the means for generating the pressurized flow of breathable gas including means for controlling the means for generating the pressurized flow of breathable gas to deliver the pressurized flow of breathable gas with a pressure that fluctuates between first and second pressure ranges, the first pressure range being higher than the second pressure range, wherein the controlling means:

- i) provides the flow of breathable gas to the airway of the subject within the first pressure range over a first time interval, wherein the first time interval spans a plurality of respiratory cycles, and
- ii) provides the flow of breathable gas to the airway of the subject at the second pressure range responsive to the following conditions being detected:
 - (a) the first time interval has elapsed, and
 - (b) a start of an expiratory flow phase has been detected.

12. The system of claim 11, wherein the means for controlling the means for generating the pressurized flow of breathable gas is further configured to provide the flow of breathable gas to the airway of the subject at the first pressure range responsive to detection of an end of the expiratory flow phase.

13. The system of claim 11, wherein the means for controlling the means for generating the pressurized flow of breathable gas provides the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval such that the pressure level is adjusted to different values within the first pressure range during different expiratory flow phases during the first time interval.

14. The system of claim 11, wherein the means for controlling the means for generating the pressurized flow of breathable gas provides the flow of breathable gas to the airway of the subject within the first pressure range over the first time interval such that the pressure level varies within 5 the first pressure range to a relatively higher pressure during inspiratory flow phases and to a relatively lower pressure during expiratory flow phases.

15. The system of claim 11, wherein the means for defining time intervals are configured such that determining 10 the amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases comprises determining the average amounts of time the subject takes to complete inspiratory flow phases and expiratory flow phases, and the time intervals are determined based on the average 15 amounts of time.

* * * * *