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(54) **N2O LIQUEFACTION SYSTEM WITH
SUBCOOLING HEAT EXCHANGER FOR
MEDICAL DEVICE**

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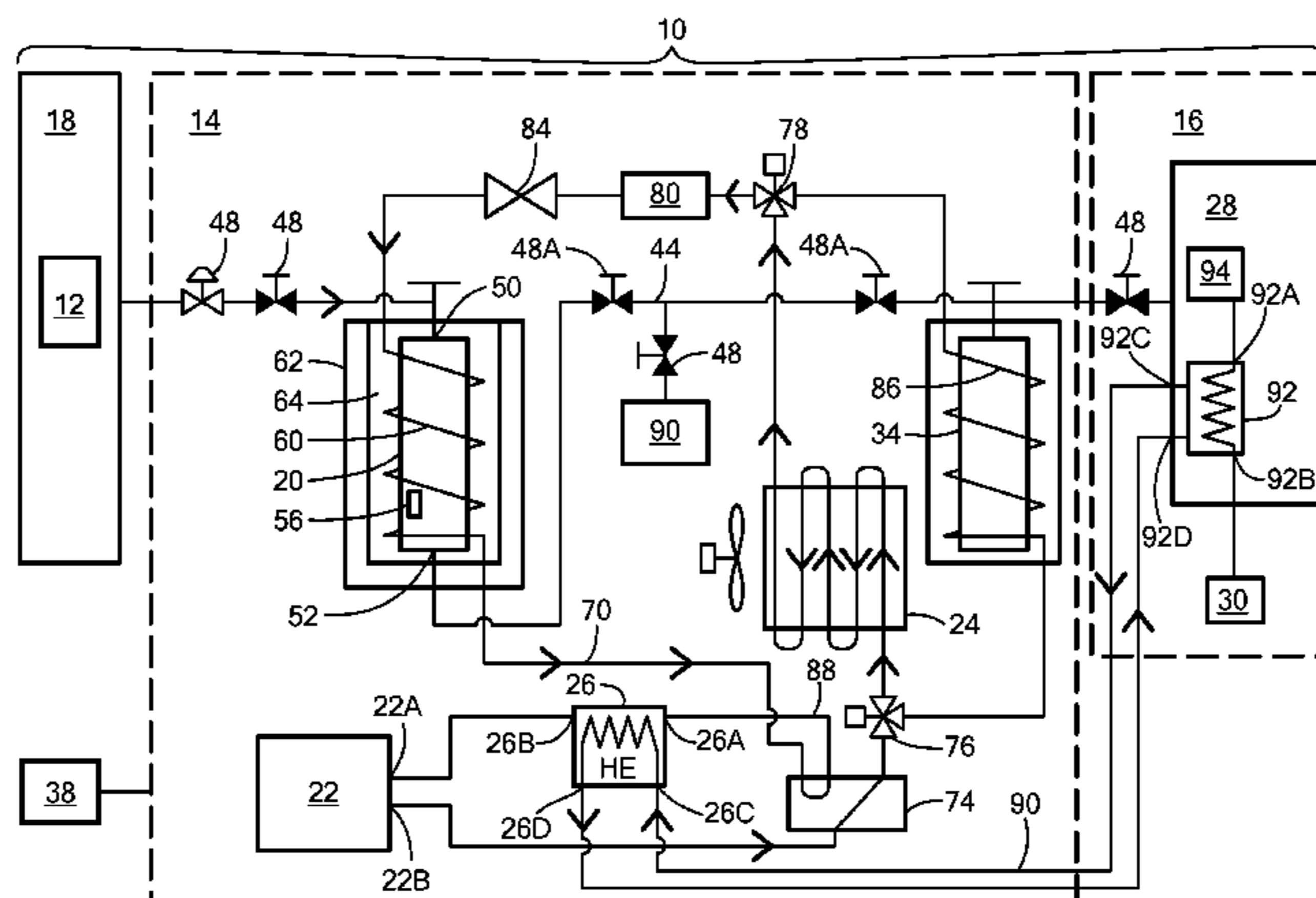
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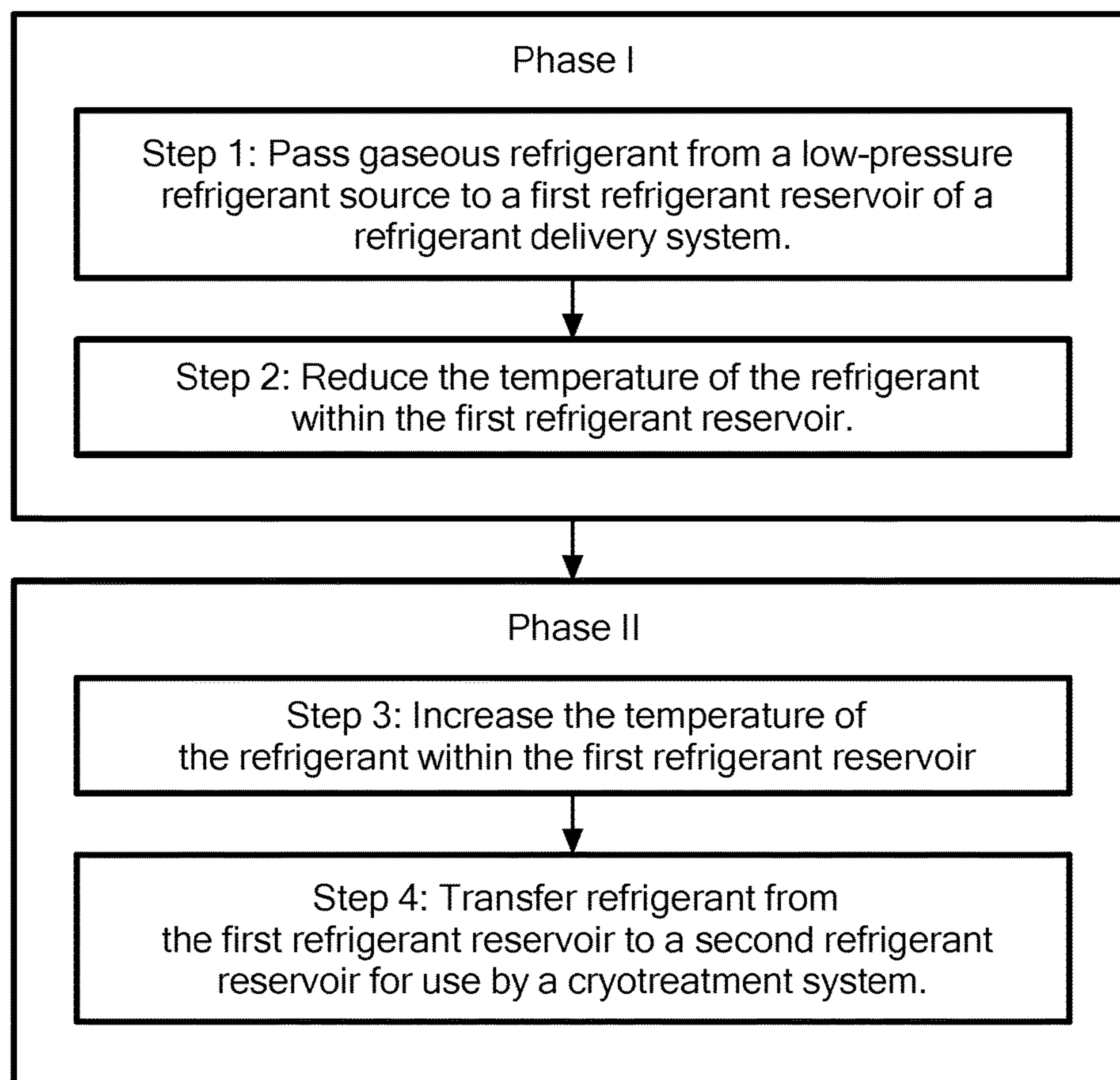
(57) **ABSTRACT**

A system and kit for using a source of low-pressure refrigerant for a cryotherapy procedure and for subcooling a cryotherapy refrigerant. The system may generally include a fluid reservoir and a fluid flow path in thermal exchange with the fluid reservoir, the fluid flow path including a first thermal exchange device in thermal exchange with the fluid reservoir, a compressor in fluid communication with the first thermal exchange device, a condenser, a reversing valve located between the compressor and the condenser, a second thermal exchange device located between the reversing valve and the compressor, and an expansion valve located between the condenser and the thermal exchange device. The third thermal exchange device may be configured to be in fluid communication with the cryotherapy console and configured to place a secondary refrigerant within the first fluid flow path in thermal communication with a secondary refrigerant of the cryotherapy system.

11 Claims, 5 Drawing Sheets



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**FIG. 1**

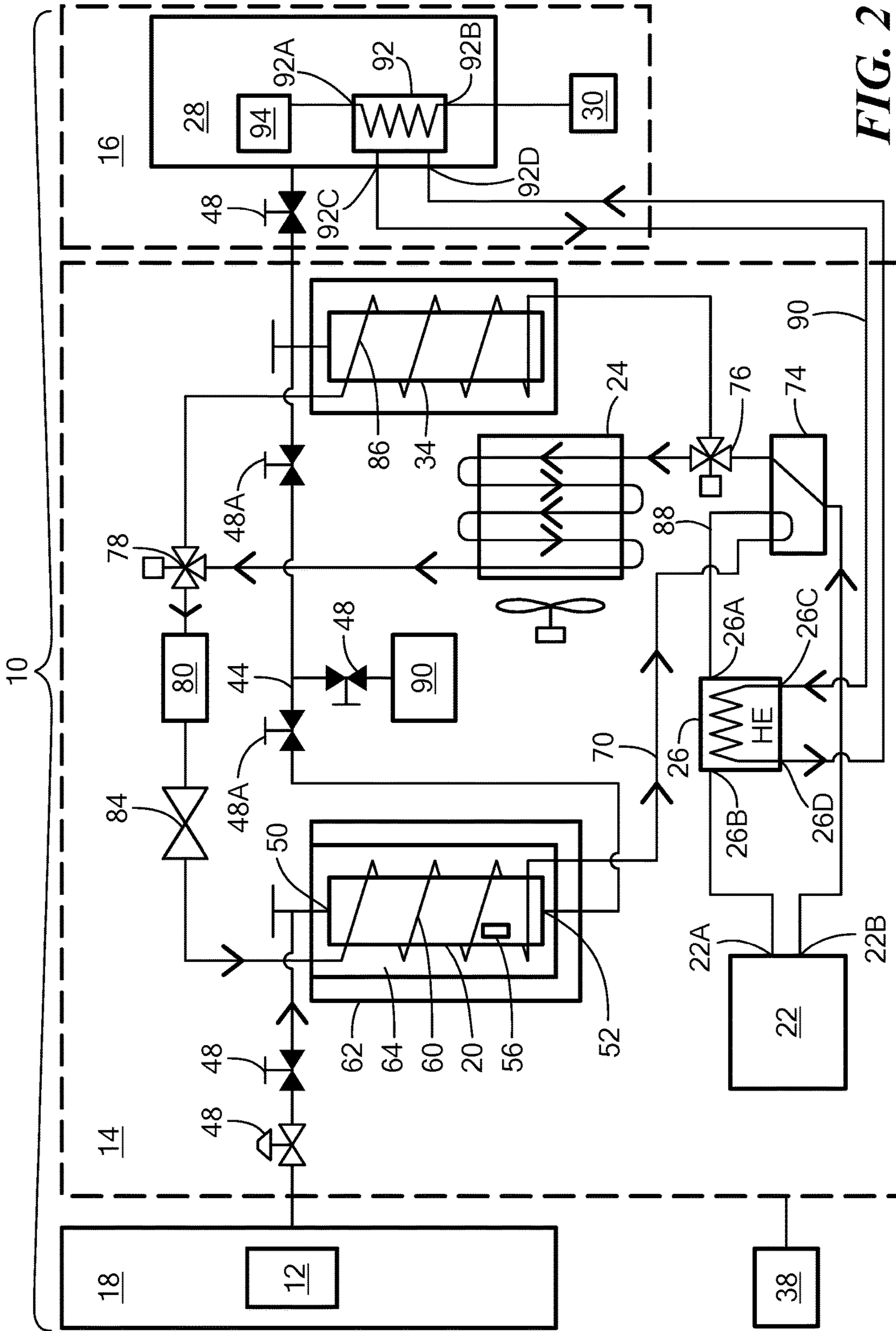


FIG. 2

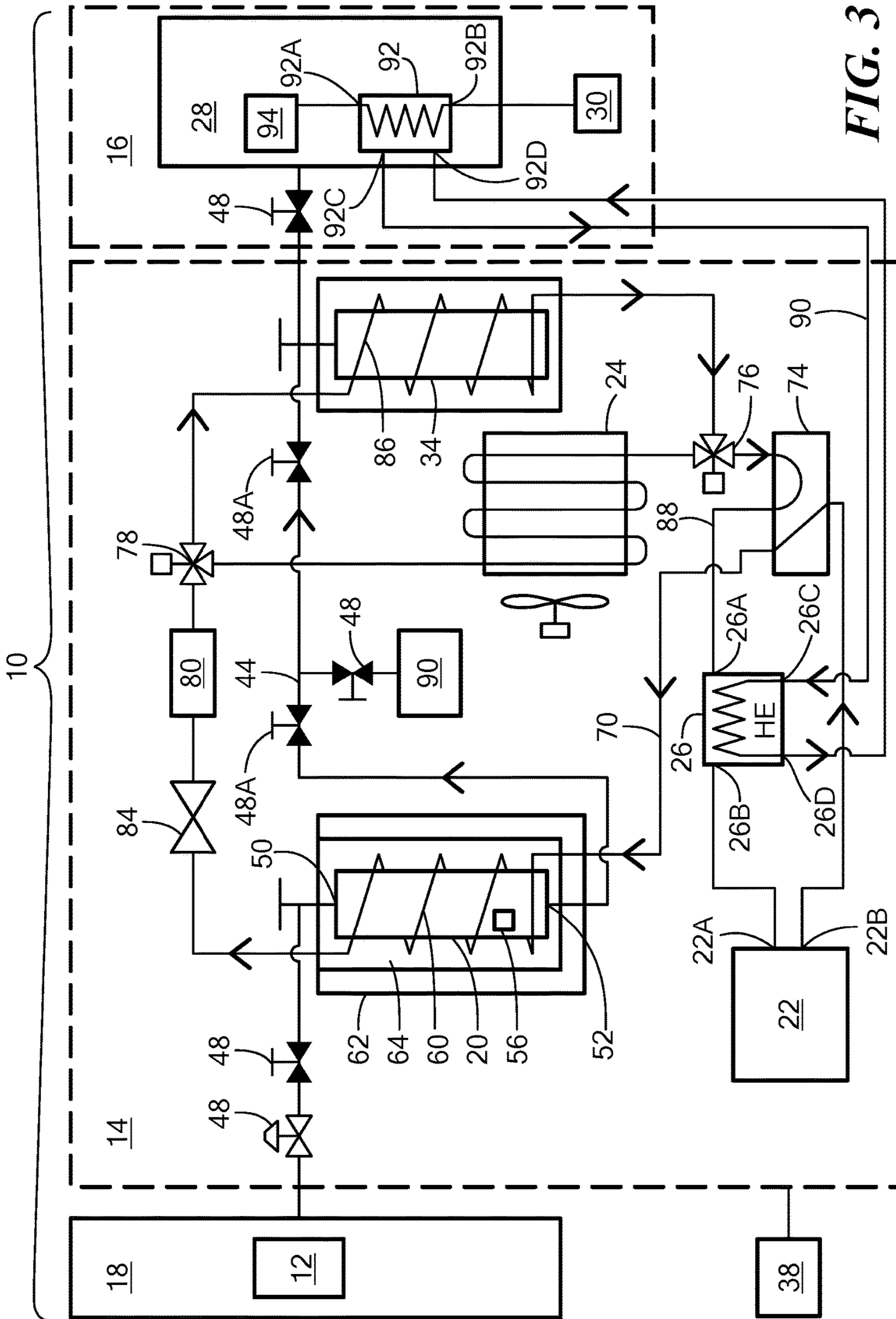


FIG. 3

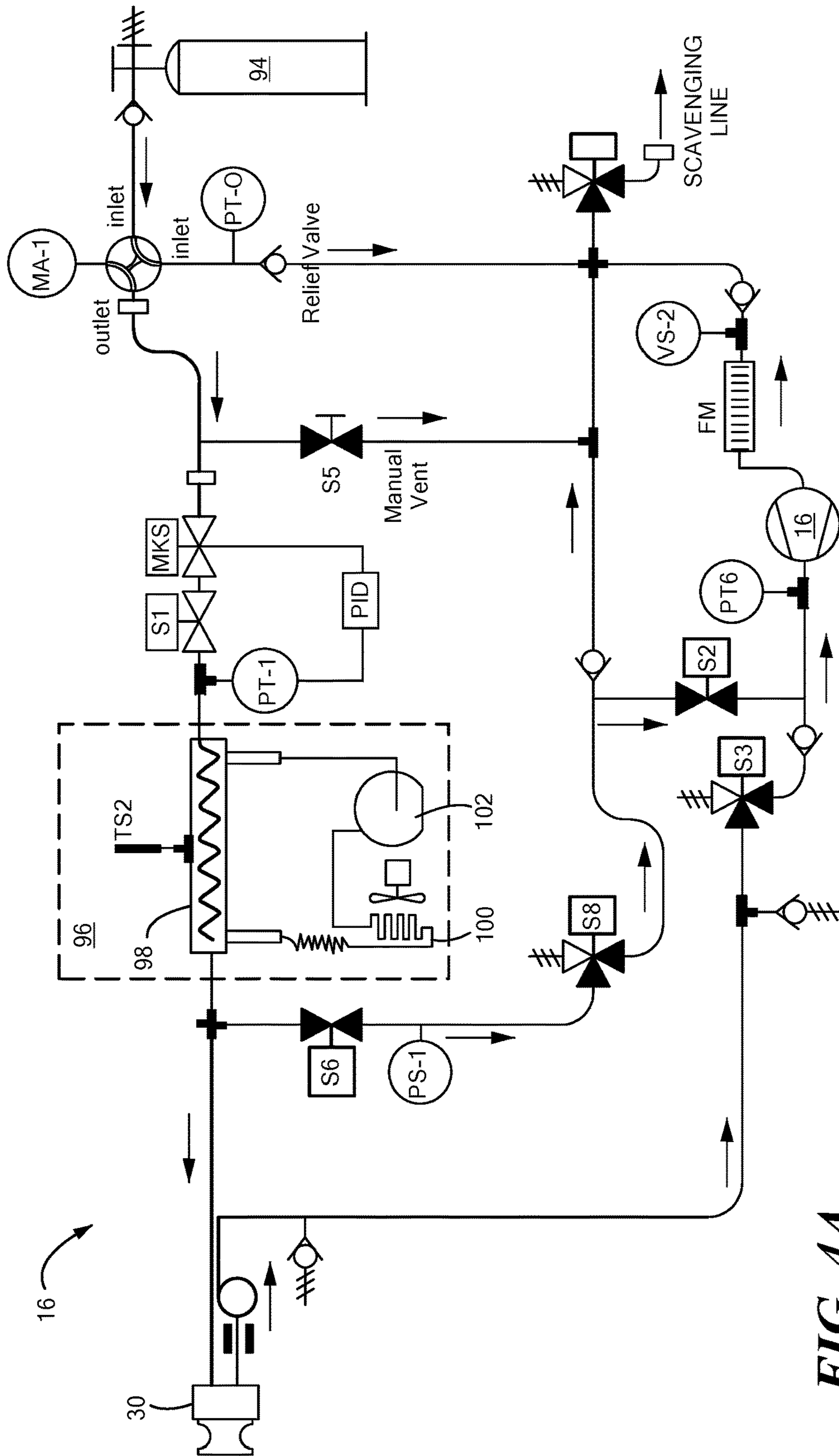


FIG. 4A
(PRIOR ART)

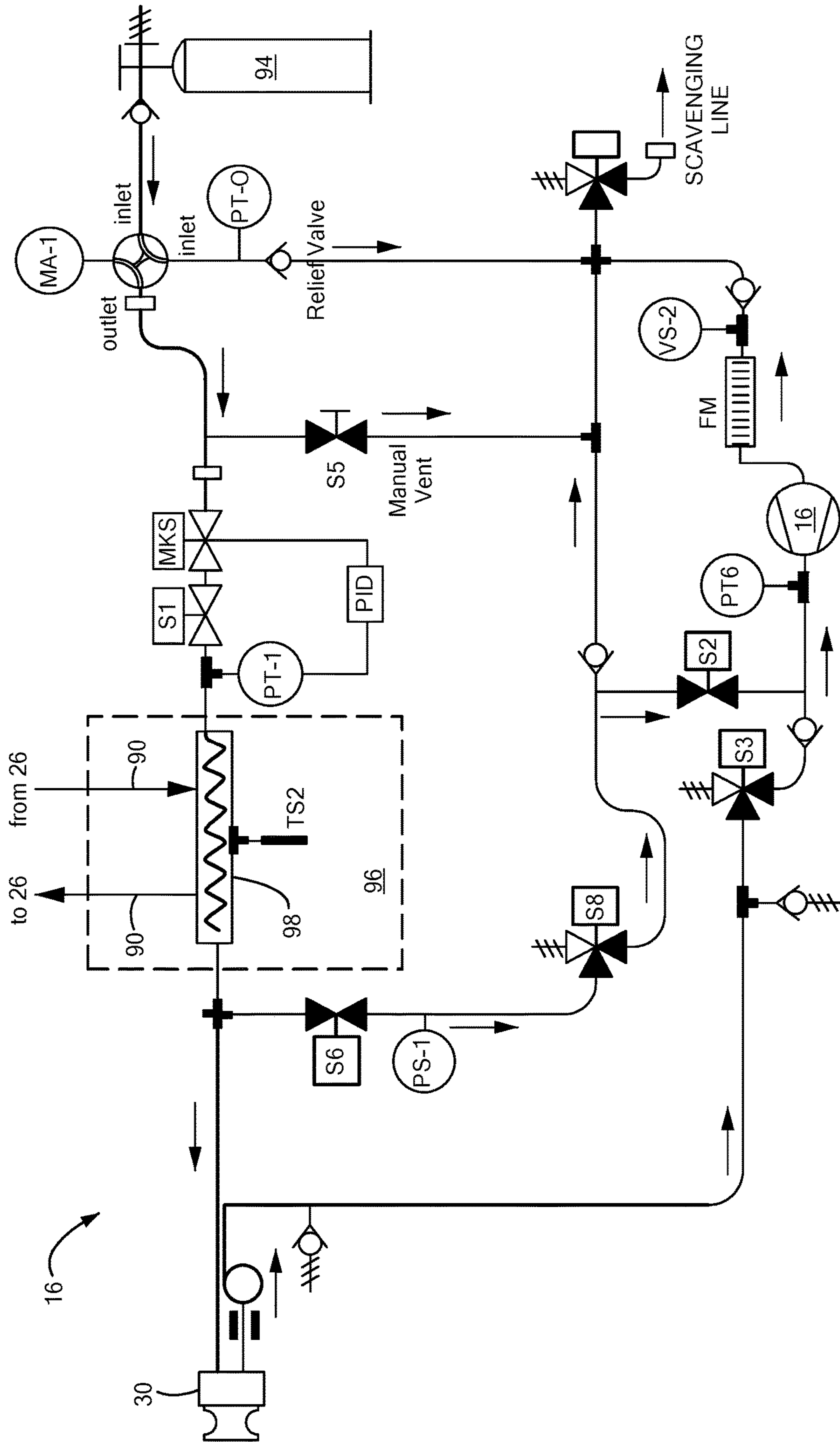


FIG. 4B

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**N₂O LIQUEFACTION SYSTEM WITH
SUBCOOLING HEAT EXCHANGER FOR
MEDICAL DEVICE**

CROSS-REFERENCE TO RELATED
APPLICATION

This application is a continuation-in-part of patent application Ser. No. 14/790,465, filed Jul. 2, 2015, entitled N₂O THERMAL PRESSURIZATION SYSTEM BY COOLING, the entirety of which is incorporated herein by reference.

STATEMENT REGARDING FEDERALLY
SPONSORED RESEARCH OR DEVELOPMENT

n/a

TECHNICAL FIELD

The present invention relates to a system and method of using a source of low-pressure refrigerant for a cryotherapy procedure. Specifically, the present invention relates to a system and method of pressurizing a source of low-pressure refrigerant by manipulating the temperature of the refrigerant and for sub-cooling a refrigerant within a cryotherapy system.

BACKGROUND

Cryotherapy includes variety of techniques used to treat and/or map tissue, and is commonly used for procedures involving cardiac tissue. Certain types of cryotherapy, such as cryoablation, involves the use of pressurized refrigerant, which is allowed to expand within, and thereby cool tissue adjacent to, the distal portion of the treatment device. The pressurized refrigerant is typically stored in a pressurized tank or cylinder in the console of the system. Although the tank is easily removed and replaced when the refrigerant source runs out, it would be more economical to refill the tank with a new supply of refrigerant. Additionally, the pressurized tanks are considered to be Dangerous Goods, and it would therefore be desirable to reduce the amount of transport, handling, and storage of refrigerant tanks used for cryotherapy procedures.

Many medical facilities, especially hospitals, include a native or in-facility, integrated source of nitrous oxide (N₂O), which is commonly used as an anesthetic. Nitrous oxide may also be used as a refrigerant in cryotherapy systems. However, the native nitrous oxide is typically stored at approximately 50 psig, which is considered a low-pressure environment. At this pressure, the nitrous oxide is unsuitable for use in a cryotherapy system and must first be pressurized and safely transferred to the cryotherapy system refrigerant reservoir. The low-pressure refrigerant cannot be used in a cryotherapy system if the refrigerant is simply compressed, since the refrigerant must also be cooled to a temperature suitable for use in the cryotherapy system.

Additionally, current consoles, such as the Gen V Cryo-Console (Medtronic, Inc., Minneapolis, Minn.), include an independent refrigeration circuit used to subcool nitrous oxide before it enters a cryotherapy device. However, including the components of the independent refrigeration circuit necessitates a larger and more complex console.

It is therefore desirable to provide a method and system for pressurizing a low-pressure source of refrigerant and safely transferring the pressurized refrigerant to a cryotherapy system. It is further desirable to provide a refrigerant

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delivery system that includes a pressurization system that provides an interface between a low-pressure refrigerant source and a cryotherapy system. It is further desirable to provide a pressurization system that includes means for subcooling nitrous oxide before it enters a treatment device of the cryotherapy system, as this would allow for the removal of the independent refrigeration circuit from the console of the cryotherapy system.

SUMMARY

The present invention advantageously provides a method and system for using a source of low-pressure refrigerant for a cryotherapy procedure. The system or kit for use with a source of low-pressure refrigerant may generally include a fluid reservoir and a closed-loop fluid flow path in thermal exchange with the fluid reservoir, the closed-loop fluid flow path including: a first thermal exchange device in thermal exchange with and fluidly isolated from the fluid reservoir; a compressor in fluid communication with the first thermal exchange device; a condenser; a reversing valve located between the compressor and the condenser; and a second thermal exchange device located between the reversing valve and the compressor. The second thermal exchange device may be configured to be in fluid communication with a cryotherapy console. The fluid flow path may be a first fluid flow path, and the kit may further include a second fluid flow path that is fluidly isolated from the first fluid flow path, with the fluid reservoir being included in the second fluid flow path. The kit may further include a third fluid flow path that is in fluid communication with the second thermal exchange device and the cryotherapy console. The second fluid flow path may be in fluid communication with the second thermal exchange device and in thermal communication with the third fluid flow path. The fluid reservoir may be configured to receive low-pressure refrigerant from the source of low-pressure refrigerant, and the kit may be configured to pressurize the low-pressure refrigerant by adjusting the temperature of the low-pressure refrigerant. The fluid reservoir may be a first fluid reservoir and the kit may further include a second fluid reservoir in the second fluid flow path, with the kit being configured to transfer pressurized refrigerant from the first fluid reservoir to the second fluid reservoir. The first fluid path may contain a first secondary refrigerant and the third fluid flow path may contain a second secondary refrigerant. Further, the reversing valve may be configured to selectively allow circulation of the first secondary refrigerant in one of a first direction and a second direction. The first fluid flow path may further include a first three-way valve located between the reversing valve and the condenser, the first three-way valve being configured to transfer the first secondary refrigerant: to the condenser when the reversing valve allows circulation of the first secondary refrigerant in the first direction; and to the compressor when the reversing valve allows circulation of the first secondary refrigerant in the second direction. The second fluid reservoir may be in thermal exchange with the third thermal exchange device, with the first fluid flow path further including a second three-way valve located between the condenser and the expansion valve, the second three-way valve being configured to transfer the first secondary refrigerant: to the expansion valve when the reversing valve allows circulation of the secondary refrigerant in the first direction; and to the third thermal exchange device when the reversing valve allows circulation of the secondary refrigerant

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erant in the second direction. The second fluid flow path may further include a vacuum source located downstream of the first fluid reservoir.

A system or kit for use with a source of low-pressure refrigerant and a cryotherapy system may generally include: a first fluid flow path and a closed-loop second fluid flow path. The first fluid flow path may include: a first fluid reservoir configured to receive a low-pressure refrigerant from the low-pressure refrigerant source; and a second fluid reservoir configured to receive a pressurized refrigerant from the first fluid reservoir. The closed-loop second fluid flow path may include: a first thermal exchange device in thermal exchange with the first fluid reservoir; a second thermal exchange device in thermal exchange with the second fluid reservoir; a compressor in fluid communication with the first thermal exchange device; a condenser; a reversing valve located between the compressor and the condenser, the reversing valve being configured to selectively allow circulation of the secondary refrigerant in one of a first direction and a second direction; a third thermal exchange device located between the reversing valve and the compressor; a first three-way valve located between the reversing valve and the condenser; an expansion valve located between the condenser and the first thermal exchange device; and a second three-way valve located between the condenser and the expansion valve; and a third fluid flow path in communication with the third thermal exchange device and configured to be in fluid communication with the cryotherapy system, the third thermal exchange device being configured to place the secondary refrigerant of the second fluid flow path in thermal communication with a secondary cryotherapy refrigerant of the cryotherapy system. The first three-way valve may be configured to transfer the secondary refrigerant to the condenser when the reversing valve allows circulation of the secondary refrigerant in the first direction, and the first three-way valve being configured to transfer the secondary refrigerant to the compressor when the reversing valve allows circulation of the secondary refrigerant in the second direction, and the second three-way valve may be configured to transfer the secondary refrigerant to the expansion valve when the reversing valve allows circulation of the secondary refrigerant in the first direction, and the second three-way valve being configured to transfer the secondary refrigerant to the second thermal exchange device when the reversing valve allows circulation of the secondary refrigerant in the second direction. Circulation of the secondary refrigerant in the first direction may reduce the temperature of the low-pressure refrigerant within the first fluid reservoir. Conversely, circulation of the secondary refrigerant in the second direction may increase the temperature and the pressure of the low-pressure refrigerant within the first fluid reservoir.

A kit for subcooling a secondary refrigerant of a cryotherapy system may include: a first fluid flow path, a closed-loop second fluid flow path that is fluidly isolated from the first fluid flow path, and a closed-loop third fluid flow path configured to be in fluid communication with the cryotherapy system. The first fluid flow path may include: a first fluid reservoir; and a second fluid reservoir configured to receive a pressurized refrigerant from the first fluid reservoir. The closed-loop second fluid flow path may contain a secondary refrigerant and may include: a first thermal exchange device in thermal communication with the first fluid reservoir; a second thermal exchange device in thermal communication with the second fluid reservoir; a compressor in fluid communication with the first thermal exchange device; a condenser; a reversing valve located between the

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compressor and the condenser, the reversing valve being configured to selectively allow circulation of the secondary refrigerant in one of a first direction and a second direction; and a third thermal exchange device located between the reversing valve and the compressor. The closed-loop third fluid flow path may be in fluid communication with the third thermal exchange device and configured to be in fluid communication with the cryotherapy system, may contain a secondary refrigerant of the cryotherapy system, and may be configured to place the secondary refrigerant within the second fluid flow path in thermal communication with the secondary refrigerant within the third fluid flow path. The secondary refrigerant within the second fluid flow path may subcool the secondary refrigerant within the third fluid flow path. The kit may further include: a first three-way valve located between the reversing valve and the condenser; an expansion valve located between the condenser and the first thermal exchange device; and a second three-way valve located between the condenser and the expansion valve. The first three-way valve may be configured to transfer the secondary refrigerant to the condenser when the reversing valve allows circulation of the secondary refrigerant in the first direction, and the first three-way valve may be configured to transfer the secondary refrigerant to the compressor when the reversing valve allows circulation of the secondary refrigerant in the second direction. Further, the second three-way valve may be configured to transfer the secondary refrigerant to the expansion valve when the reversing valve allows circulation of the secondary refrigerant in the first direction, and the second three-way valve may be configured to transfer the secondary refrigerant to the second thermal exchange device when the reversing valve allows circulation of the secondary refrigerant in the second direction.

BRIEF DESCRIPTION OF THE DRAWINGS

A more complete understanding of the present invention, and the attendant advantages and features thereof, will be more readily understood by reference to the following detailed description when considered in conjunction with the accompanying drawings wherein:

FIG. 1 shows a flow chart for a method of refrigerant delivery from a low-pressure native refrigerant source to a cryotherapy system;

FIG. 2 shows a schematic representation of a refrigerant delivery system, with a secondary refrigerant flowing through a fluid flow path in a first direction;

FIG. 3 shows a schematic representation of the refrigerant delivery system, with a secondary refrigerant flowing through the fluid flow path in a second direction;

FIG. 4A shows a schematic representation of a prior art cryotherapy system having an independent refrigeration circuit; and

FIG. 4B shows a schematic representation of a cryotherapy system in accordance with the present invention.

DETAILED DESCRIPTION

Referring now to FIGS. 1-3, a flow chart for a method of refrigerant delivery from a low-pressure, native refrigerant source to a cryotherapy device is shown in FIG. 1 and schematic representations of a refrigerant delivery system are shown in FIGS. 2 and 3. In FIGS. 2 and 3, a schematic representation of a refrigerant delivery system is shown, the refrigerant delivery system 10 including a low-pressure refrigerant source 12 in fluid communication with a pressurization system 14 and a cryotherapy system 16. The

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low-pressure refrigerant source **12** may generally include a volume of refrigerant stored in a low-pressure environment within or at a medical facility **18**, the pressurization system **14** may generally include a first refrigerant reservoir **20**, a compressor **22**, a condenser **24**, and a heat exchanger **26**, and the cryotherapy system **16** may generally include a console **28**, a cryotherapy device **30**. The refrigerant delivery system **10** may also include a second refrigerant reservoir **34**, although this reservoir **34** may be considered to be part of the pressurization system **14** or the cryotherapy system **16**, depending on the configuration of the pressurization system **14**.

The pressurization system **14** may further include one or more processors **38** in communication with various components of the pressurization system **14** and, optionally, with the low-pressure refrigerant source **12** and/or the cryotherapy system **16**. For example, the pressurization system **14** may include one or more processors **38** that are capable of transmitting, receiving, and/or processing data for system monitoring and control. As a non-limiting example, the pressurization system **14** may include one or more processors **38** for the automatic or semi-automatic control of the pressurization system **14**, such as automatic or semi-automatic control of system valves. For simplicity, a processor **38** is shown in the figures as generally being in communication with the pressurization system **14**, although it will be understood as noted above that the one or more processors **38** may be in communication with one or more specific components of the low-pressure refrigerant source **12**, the pressurization system **14**, and/or the cryotherapy system **16**.

The first refrigerant reservoir **20** may be in fluid communication with a medical facility's refrigerant source. The term "medical facility" may refer to any facility that includes a source of refrigerant, including hospitals, walk-in clinics, and other facilities. Although a cryotherapy system **16** may be used in medical facilities, it will be understood that the method shown and described herein of pressurizing a refrigerant source for delivery to a given device may be adapted for use in other industries in addition to the medical industry.

Hospitals and other medical facilities commonly include a source of refrigerant, such as nitrous oxide (N_2O), that is stored as a gas at a normal working pressure of, for example, approximately 50 psig. Although different medical facilities may use various storage methods, a typical scheme is to store the gaseous N_2O in large tanks connected to a manifold, which regulates the pipeline pressure to the normal working pressure (for example, approximately 50 psig). The N_2O pipeline may be connected or connectable to any of a variety of medical systems and/or devices. Although this low-pressure source of refrigerant (which may also be referred to herein as a "native source of refrigerant" or "native source of N_2O ") may provide an easily accessible supply of N_2O for a cryotherapy procedure, the low-pressure N_2O may have to be pressurized and liquefied before can be used in a cryotherapy system **16**, a process that is discussed in more detail below.

The method shown in FIG. **1** may generally include two phases: Phase I in which a gaseous, low-pressure refrigerant is cooled and liquefied and stored in a first refrigerant reservoir **20** and Phase II in which the liquefied refrigerant is warmed and pressurized to facilitate movement of the refrigerant from the first refrigerant reservoir **20** to a second refrigerant reservoir **34**.

In the first step **110** of the method, in Phase I, a gaseous refrigerant from a low-pressure refrigerant source **12** may pass along a first fluid flow path **44** to the first fluid reservoir

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20 of the pressurization system **14**. The first fluid flow path **44** may be a closed-loop flow path. As is discussed above, the low-pressure refrigerant source **12** may be a native source of refrigerant, such as N_2O , located within a medical facility. The first fluid flow path **44** may include one or more valves **48** for metering flow of the refrigerant from the low-pressure refrigerant source **12** to the first refrigerant reservoir **20**. Although the first refrigerant reservoir **20** may be of any size, shape, and configuration, it may, for example, have a cylindrical shape with a fluid inlet **50** at a first end and a fluid outlet **52** at a second end.

Once the refrigerant is transferred from the low-pressure refrigerant source **12** to the first refrigerant reservoir **20**, the temperature of the refrigerant may then be reduced in order to liquefy the gaseous refrigerant in the second step **120** of the method. Liquefying the gaseous refrigerant may reduce the pressure of the refrigerant, thereby allowing a greater amount of refrigerant to be stored within the first refrigerant reservoir **20**. Refrigerant may continue to be added to the first refrigerant reservoir **20** until a pressure of the liquid refrigerant within the first refrigerant reservoir **20** becomes equalized with a pressure of the gaseous refrigerant upstream of the first refrigerant reservoir **20**. To monitor pressure equalization, one or more pressure, temperature, or other sensors **56** may be included in the low-pressure refrigerant source **12**, the first refrigerant reservoir **20**, and/or within the first fluid flow path **44** between the low-pressure refrigerant source **12** and the first refrigerant reservoir **20**. During Phase I, one or more valves **48A** between the first refrigerant reservoir **20** and the second refrigerant reservoir **34** may be closed so that refrigerant cannot flow into the second refrigerant reservoir **34**.

The first refrigerant reservoir **20** may be in a thermal exchange relationship (that is, in thermal communication) with a first thermal exchange device **60**. As a non-limiting example, the first thermal exchange device **60** may be an evaporator having a coiled configuration and may be wrapped one or more times about a circumference of the first refrigerant reservoir **20**. The first refrigerant reservoir **20** and the first thermal exchange device **60** may together be located within an insulating container **62**. The insulating container **62** may be at least partially composed of a material or layers of materials that prevent or reduce the transmission of heat. Additionally, the insulating container **62** may be filled with, and the first thermal exchange device **60** and the first refrigerant reservoir **20** may be surrounded by, a nonfreezing liquid **64** such as methanol, propylene glycol, or other liquid having similar properties. The nonfreezing liquid **64** may improve heat transfer between the first thermal exchange device **60** and the first refrigerant reservoir **20**. Thus, the first thermal exchange device **60** may cool the refrigerant within the first refrigerant reservoir **20** and the insulating container **62** may improve cooling efficiency. The insulating container **62** may have a shape and configuration similar to that of the first refrigerant reservoir **20**, and may be sized just large enough to accommodate the first refrigerant reservoir **20**, first thermal exchange device **60**, and nonfreezing liquid **64** therein. Further, the first refrigerant reservoir **20** optionally may be integrated within the insulating container **62**.

In order to reduce the temperature of the refrigerant within the first refrigerant reservoir **20** with the first thermal exchange device **60**, a secondary refrigerant may be circulated through the first thermal exchange device **60**. This secondary refrigerant may flow through a second fluid flow path **70** that is different than the first fluid flow path **44** of the refrigerant from the low-pressure refrigerant source **12** to the cryotherapy system **16**. Put simply, the circulation of the

secondary refrigerant within the second fluid flow path 70 may operate to selectively cool or warm refrigerant within the first fluid flow path 44. The secondary refrigerant may be a refrigerant that has an evaporation temperature of -45°C . or lower. As a non-limiting example, the secondary refrigerant may be R508B or R23. From the first thermal exchange device 60, the gaseous secondary refrigerant may flow through a second fluid flow path 70 and through a reversing or four-way valve 74. As is described in more detail below, operation of the reversing valve 74 may allow for the selective cooling (when in a standard-flow configuration, shown in FIG. 2) or warming (when in a reverse-flow configuration, shown in FIG. 3) of the refrigerant within the first refrigerant reservoir 20.

While still in Phase I, the gaseous secondary refrigerant may pass from the reversing valve 74 to the compressor 22. The compressor 22 may be, for example, a hermetic (also referred to as a “hermetically sealed”) compressor that is configured to compress the secondary refrigerant, thereby increasing the pressure and temperature, and decreasing the volume, of the secondary refrigerant. The compressed secondary refrigerant may then pass from the compressor 22 and back through the reversing valve 74 to a first three-way valve 76. When the pressurization system 14 is in the standard-flow configuration, the first three-way valve 76 may be configured such that the secondary refrigerant flows from the reversing valve 74, through the heat exchanger 26, and to the condenser 24, such as a forced-air condenser. The condenser 24 may condense the secondary refrigerant, thereby reducing the temperature of and liquefying the high-pressure secondary refrigerant.

From the condenser 24, the secondary refrigerant may pass through a second three-way valve 78. When the pressurization system 14 is in the standard-flow configuration, the second three-way valve 78 may be configured such that secondary refrigerant passes from the condenser 24 to a filter-dryer 80. The filter-dryer 80 may be, for example, a moisture separator, a desiccant dryer, or the like. From the filter-dryer 80, the secondary refrigerant may pass through a metering device, such as an expansion valve 84. The flow of the liquid secondary refrigerant into the first thermal exchange device 60 may be metered by the expansion valve 84 such that the secondary refrigerant evaporates within the first thermal exchange device 60 and becomes a cold gas. The gaseous secondary refrigerant then may pass from the expansion valve 84 back to the first thermal exchange device 60. As discussed above, the secondary refrigerant within the first thermal exchange device 60 may reduce the temperature of the refrigerant within the first refrigerant reservoir 20. Once the first refrigerant reservoir 20 is full of refrigerant (that is, once a pressure within the first refrigerant reservoir 20 becomes equalized with a pressure of the refrigerant upstream of the first refrigerant reservoir 20), Phase II of the method may begin.

In Phase II, refrigerant from the first refrigerant reservoir 20 may be transferred to the second refrigerant reservoir 34. The second refrigerant reservoir 34 may be in thermal communication with a second thermal exchange device 86, and both may be included in the pressurization system 14. Alternatively, the second thermal exchange device 86 may be included in the pressurization system 14, and the second thermal exchange device 86 may be configured such that it can be placed in thermal exchange with a second refrigerant reservoir 34 that is included in the cryotherapy system 16. Alternatively, the second refrigerant reservoir 34 and the second thermal exchange device 86 may both be a part of the cryotherapy system 16. In this case, the second fluid flow

path 70 of the pressurization system 14 may be configured to be fluidly connected to one or more components of the cryotherapy system 16, such as the second thermal exchange device 86 in thermal exchange with the second refrigerant reservoir 34. The second refrigerant reservoir 34 may be sized and configured to fit within the cryotherapy system console 28, although the second refrigerant reservoir 34 may alternatively be located outside the console 28. Thus, although the second refrigerant reservoir 34 is shown in FIGS. 2 and 3 as being located outside of the console 28 for simplicity, it will be understood that the second refrigerant reservoir 34 may instead be located within the console 28.

It will be understood that the pressurization system 14 may be a kit that is adapted to be connected to both a low-pressure refrigerant source 12, such as a native nitrous oxide source at a hospital or other medical facility, and a cryotherapy system 16, including the cryotherapy console 28 and device 30. For example, the pressurization system 14 may include one or more sensors for monitoring system parameters, such as temperature and pressure. Data collected by these one or more sensors 56 may be communicated to the pressurization system processor 38 and/or the cryotherapy system console 28. Further, the pressurization system 14 processor may be in communication with the cryotherapy console 28 to exchange data. For example, the pressurization system processor 38 may send a signal to the cryotherapy console 28 when the second refrigerant reservoir 34 is full and sufficiently cooled for commencement of a cryotherapy procedure. Further, the pressurization system 14 processor may enable the automatic or semi-automatic control of the pressurization system 14, such as automatic or semi-automatic control of the reversing valve 74, expansion valve 84, and the first 76 and second 78 three-way valves.

In the third step 130 of the method, in Phase II, the temperature of the refrigerant within the first refrigerant reservoir 20 may be increased or allowed to increase in order to facilitate transfer of the refrigerant to the second refrigerant reservoir 34. For example, the flow of the secondary refrigerant within the second fluid flow path 70 may be discontinued in order to allow the temperature, and therefore the pressure, of the refrigerant within the first refrigerant reservoir 20 to gradually increase. As a non-limiting example, the temperature of the refrigerant may be allowed to increase to a temperature that is slightly higher than ambient temperature, such as approximately 30°C . ($\pm 5^{\circ}\text{C}$.) and the pressure may be allowed to increase to approximately 900 PSI (± 50 PSI). At the same time, the temperature of the pressurized refrigerant may be reduced as it is transferred to the second refrigerant reservoir 34.

Additionally or alternatively, the pressurization system 14 may include one or more valves that may increase the rate at which the pressure and temperature of the refrigerant within the first fluid is increased. For example, the reversing valve 74 of the pressurization system 14 may reverse the flow of the secondary refrigerant through the second fluid flow path 70. In Phase II, before the refrigerant is transferred from the first refrigerant reservoir 20 into the second refrigerant reservoir 34, flow of the secondary refrigerant may be reserved such that the temperature of refrigerant within the first refrigerant reservoir 20 is increased and the temperature of the refrigerant within the second refrigerant reservoir 34 as decreased.

In this reverse-flow configuration (shown in FIG. 3), secondary refrigerant may pass through the second fluid flow path 70 through the compressor 22. Warmed from the compressor 22, the secondary refrigerant may then pass to the first thermal exchange device 60, which may function

like a condenser in the reverse-flow configuration because of the low-temperature condition of the refrigerant within the first refrigerant reservoir 20 created in Phase I. As a result, the secondary refrigerant may be liquefied within the first thermal exchange device 60. Due to the thermal exchange relationship between the first thermal exchange device 60 and the first refrigerant reservoir 20, the refrigerant within the first refrigerant reservoir 20 may increase whereas the temperature of the secondary refrigerant within the first thermal exchange device 60 may decrease.

The cooled secondary refrigerant may pass from the first thermal exchange device 60 through the expansion valve 84 and the filter-dryer 80, and then through the second three-way valve 78. When the pressurization system 14 is in the reverse-flow configuration, the second three-way valve 78 may be configured such that the secondary refrigerant bypasses the condenser 24 and instead passes from the filter-dryer 80 into the second thermal exchange device 86 that is in a thermal exchange relationship with the second refrigerant reservoir 34. The liquid secondary refrigerant may evaporate within the second thermal exchange device 86 and, by virtue of the thermal exchange relationship, may cool the refrigerant within the second refrigerant reservoir 34. In some configurations, the second thermal exchange device 86 may be included in the cryotherapy system console 28 and may be in thermal exchange with the second refrigerant reservoir 34. The pressurization system 14 may be configured to be in fluid communication with existing cryotherapy systems, such as by using one or more connectors, valves, or other after-market components to connect the two systems.

Secondary refrigerant may then pass from the second thermal exchange device 86 to the first three-way valve 76. In the reverse-flow configuration, the first three-way valve 76 may be configured such that the secondary refrigerant flows from the second thermal exchange device 86, to the reversing valve 74, through the heat exchanger 26, and then to the compressor 22. Secondary refrigerant may then pass from the compressor 22 back into the first thermal exchange device 60 within the insulating container 62.

The circulation of the secondary refrigerant through the second fluid flow path 70 in the reverse-flow configuration may be discontinued once no flow is circulating through the valve 48 just upstream of the second refrigerant reservoir 28 or once a certain refrigerant level is reached inside the first refrigerant reservoir 20.

In the fourth step 140 of the method, in Phase II, the refrigerant may be transferred from the first refrigerant reservoir 20 to the second refrigerant reservoir 34. In the fourth step 140, one or more valves 48A between the first refrigerant reservoir 20 and the second refrigerant reservoir 34 may be fully or partially open to allow the refrigerant to flow from the first refrigerant reservoir 20 to the second refrigerant reservoir 34. To further facilitate the transfer, the first fluid flow path 44 may include a vacuum source 90 that creates a pressure differential within the first fluid flow path 44. In this way, refrigerant may be drawn by the vacuum source 90 from the first refrigerant reservoir 20 to the second refrigerant reservoir 34. The vacuum source 90 may also facilitate the removal of air and other impurities from the first 20 and second 34 refrigerant reservoirs before refrigerant is drawn from the first refrigerant reservoir 20. Once the refrigerant is within the second refrigerant reservoir 34, the refrigerant may be circulated through a cryotherapy device 30 used to perform a cryotherapy procedure, such as cardiac ablation and/or mapping. Circulation of the secondary refrigerant within the second fluid flow path 70 may

continue in the reverse-flow configuration during at least a part of the cryotherapy procedure, in order to maintain the pressurized refrigerant at a low temperature within the second refrigerant reservoir 34.

As is discussed above, the reversing four-way valve 74 allows for fluid flow in a standard-flow direction and a reverse-flow direction. As is shown in FIGS. 2 and 3, the secondary refrigerant passes through the heat exchanger 26 in both the standard-flow direction and the reverse-flow direction. In either flow direction, secondary refrigerant flowing through the portion 88 of the second fluid flow path 70 that enters an inlet 26A of the heat exchanger 26 is always cold as it is downstream (that is, at the outlet side) of the thermal exchange device 60 or from the second thermal exchange device 86 when acting as an evaporator. Thus, the secondary refrigerant within the thermal exchange device 26 may cool another fluid flowing within the heat exchange device 26 and that is in thermal communication with the secondary fluid.

The thermal exchange device 26 may be in fluid communication with a third fluid flow path 90 that is in fluid communication with a third thermal exchange device 92 within console 28 (shown in FIG. 4B). The third thermal exchange device 92 may include a secondary refrigerant that is fluidly isolated from, but in thermal communication with, the primary refrigerant delivered to the cryotherapy device 30. This secondary refrigerant of the cryotherapy system 16 may flow through the third fluid flow path 90 and be in thermal communication with (but fluidly isolated from) the secondary refrigerant flowing within the pressurization system 14 within the thermal exchange device 26. Thus, the thermal exchange device 26 within the pressurization system 14 may reduce the temperature of a secondary refrigerant of the cryotherapy system 16. In turn, the cooled secondary refrigerant of the cryotherapy system 16 may subcool the primary refrigerant within the third thermal exchange device 92 of the cryotherapy system 16. As is shown in FIG. 4B, the first secondary refrigerant may enter a first inlet 26A of the thermal exchange device 26, exit a first outlet 26B of the thermal exchange device 26, enter an inlet 22A of the compressor 22, and exit an outlet 22B of the compressor 22. The secondary refrigerant of the cryotherapy system 16 may enter a second inlet 26C of the thermal exchange device 26 and exit a second outlet 26D of the thermal exchange device 26. Within the cryotherapy system 16, the primary refrigerant may 20 pass from a fluid reservoir 94 into a first inlet 92A of the third thermal exchange device 92, within which the primary refrigerant is subcooled by the secondary refrigerant within the third fluid flow path 90, out a first outlet 92B of the third thermal exchange device 92, and into the cryotherapy device 30. Likewise, the secondary refrigerant within the third fluid flow path may enter a second inlet 92C of the third thermal exchange device 92, and may exit from a second outlet 92D of the thermal exchange device. Although not shown in FIGS. 2 and 3, it will be understood that the primary refrigerant of the cryotherapy system 16 may pass through various other system components, such as those shown in FIG. 4B.

As is shown in FIG. 4A, currently known cryotherapy systems may include consoles having an independent refrigeration circuit 96, which may include a thermal exchange device 98, a condenser 100, and a compressor 102. By including the thermal exchange device 26 within the pressurization system 14, the condenser 100, compressor 102, and other components (for example, valves, tubing, and a compressor fan) can be removed from the console (as shown in FIG. 4B). It will be understood that the cryotherapy

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system 16 in use with the pressurization system 14 may not be exactly as shown in FIGS. 4A and 4B.

It will be understood that the medical facility, pressurization system 14, and/or the cryotherapy system 16 may include system components in addition to those shown in the figures, such as one or more valves, computers, processors, fluid reservoirs, user input devices, sensors, vacuum sources, power generators, or the like. Although not shown, the pressurization system 14 may include one or more temperature sensors and/or pressure sensors located throughout the system for monitoring fluid temperature within the first and/or second fluid flow path 70. Additionally, the pressurization system 14 and/or the cryotherapy system 16 may include one or more displays, audio alerts, visual alerts, or the like for communicating system conditions to a user. Further, it will be understood that although each of the second fluid flow path 70 components of the pressurization system 14 may include an inlet port and an outlet port, whether each port functions as an inlet or an outlet may be determined by whether the second fluid flow path 70 is operating in the standard-flow configuration or the reverse-flow configuration.

It will be appreciated by persons skilled in the art that the present invention is not limited to what has been particularly shown and described herein above. In addition, unless mention was made above to the contrary, it should be noted that all of the accompanying drawings are not to scale. A variety of modifications and variations are possible in light of the above teachings without departing from the scope and spirit of the invention, which is limited only by the following claims.

What is claimed is:

1. A kit for use with a source of low-pressure refrigerant, the kit comprising:
 - a fluid reservoir;
 - a first closed-loop fluid flow path in thermal exchange with the fluid reservoir, the first closed-loop fluid flow path including:
 - a first thermal exchange device in thermal exchange with and fluidly isolated from the fluid reservoir;
 - a compressor in fluid communication with the first thermal exchange device; a condenser;
 - a reversing valve located between the compressor and the condenser; and a second thermal exchange device located between the reversing valve and the compressor;
 - a second fluid flow path that is fluidly isolated from the first closed-loop fluid flow path, the fluid reservoir being included in the second fluid flow path; and

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a third fluid flow path, the third fluid flow path being in fluid communication with the second thermal exchange device and a cryotherapy console.

2. The kit of claim 1, wherein the second thermal exchange device is configured to be in fluid communication with the cryotherapy console.

3. The kit of claim 1, wherein the second fluid flow path is in fluid communication with the second thermal exchange device and in thermal communication with the third fluid flow path.

4. The kit of claim 3, wherein the fluid reservoir is configured to receive low-pressure refrigerant from the source of low-pressure refrigerant.

5. The kit of claim 3, wherein the kit is configured to pressurize the low-pressure refrigerant by adjusting the temperature of the low-pressure refrigerant.

6. The kit of claim 5, wherein the fluid reservoir is a first fluid reservoir, the kit further comprising a second fluid reservoir in the second fluid flow path, the kit being configured to transfer pressurized refrigerant from the first fluid reservoir to the second fluid reservoir.

7. The kit of claim 6, wherein the first fluid flow path contains a first secondary refrigerant and the third fluid flow path contains a second secondary refrigerant.

8. The kit of claim 7, wherein the reversing valve is configured to selectively allow circulation of the first secondary refrigerant in one of a first direction and a second direction.

9. The kit of claim 8, wherein the first fluid flow path further includes a first three-way valve located between the reversing valve and the condenser, the first three-way valve being configured to transfer the first secondary refrigerant: to the condenser when the reversing valve allows circulation of the first secondary refrigerant in the first direction; and

to the compressor when the reversing valve allows circulation of the first secondary refrigerant in the second direction.

10. The kit of claim 9, wherein the second fluid reservoir is in thermal exchange with a third thermal exchange device, the first fluid flow path further including a second three-way valve located between the condenser and the expansion valve, the second three-way valve being configured to transfer the first secondary refrigerant:

to the expansion valve when the reversing valve allows circulation of the secondary refrigerant in the first direction; and

to the third thermal exchange device when the reversing valve allows circulation of the secondary refrigerant in the second direction.

11. The kit of claim 3, wherein the second fluid flow path further includes a vacuum source in located downstream of the first fluid reservoir.

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