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(12) **United States Patent**  
**Sanders et al.**

(10) **Patent No.:** **US 10,278,734 B2**  
(45) **Date of Patent:** **May 7, 2019**

(54) **CLAMPING DEVICE FOR USE WITH AN ANATOMIC EXTERNAL FIXATION DEVICE**

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(21) Appl. No.: **15/701,104**

(22) Filed: **Sep. 11, 2017**

(65) **Prior Publication Data**

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**Related U.S. Application Data**

(63) Continuation of application No. 15/359,479, filed on Nov. 22, 2016, now Pat. No. 9,867,637, which is a continuation-in-part of application No. 14/871,618, filed on Sep. 30, 2015, now Pat. No. 9,597,117.

(60) Provisional application No. 62/058,262, filed on Oct. 1, 2014.

(51) **Int. Cl.**  
**A61B 17/64** (2006.01)

(52) **U.S. Cl.**  
CPC ..... **A61B 17/6416** (2013.01); **A61B 17/6425** (2013.01); **A61B 17/6458** (2013.01); **A61B 17/6466** (2013.01); **A61B 17/645** (2013.01)

(58) **Field of Classification Search**  
CPC ..... Y10T 24/4441; Y10T 244/4513; A61B 17/6416

See application file for complete search history.

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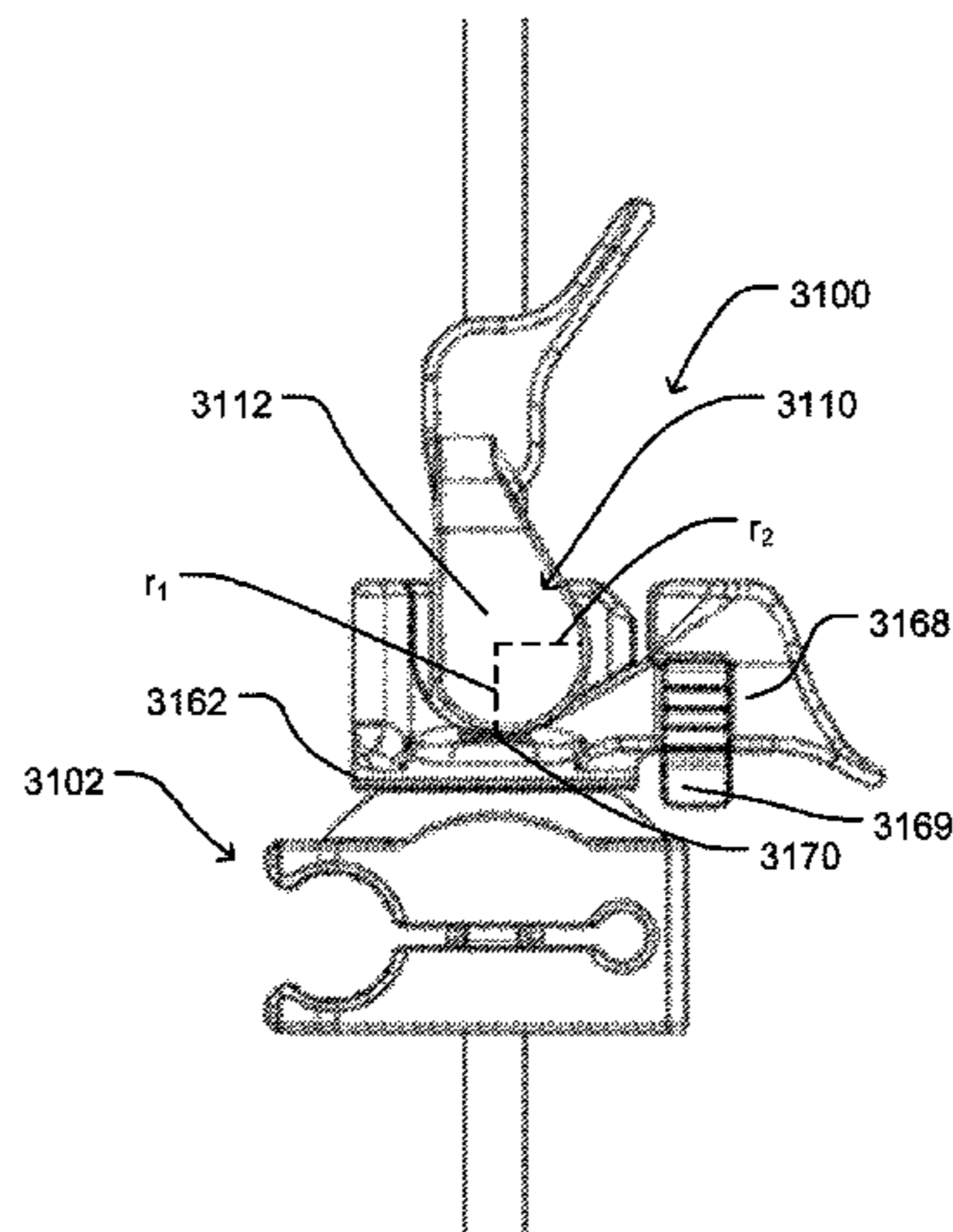
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*Assistant Examiner* — Tara Rose E Carter  
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(57) **ABSTRACT**

A clamping device includes a clamp body and a locking assembly. The clamp body includes a first jaw defining a first opening and a second jaw defining a second opening. The locking assembly includes a first locking element, a second locking element, and a lever. The first locking element includes a first end and a shaft portion extending from the first end. The shaft portion is sized to pass through the first opening and the second opening. The locking assembly is configured to reduce a distance between the first jaw and the second jaw responsive to rotation of the second locking element. The lever is configured to attach to the second locking element and rotate about the second locking element from a first position to a second position to cause the distance between the first jaw and the second jaw to be reduced further.

**18 Claims, 63 Drawing Sheets**



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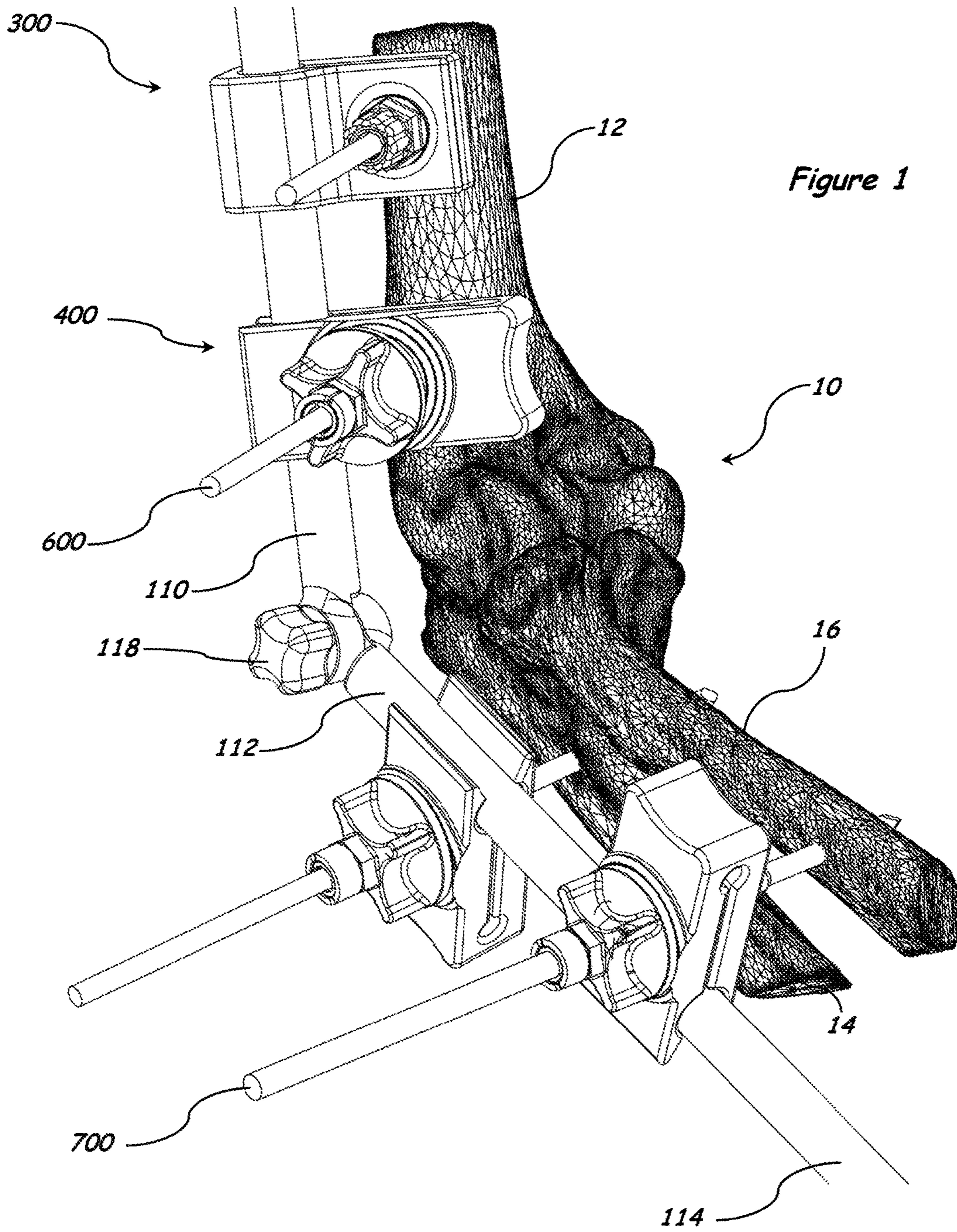
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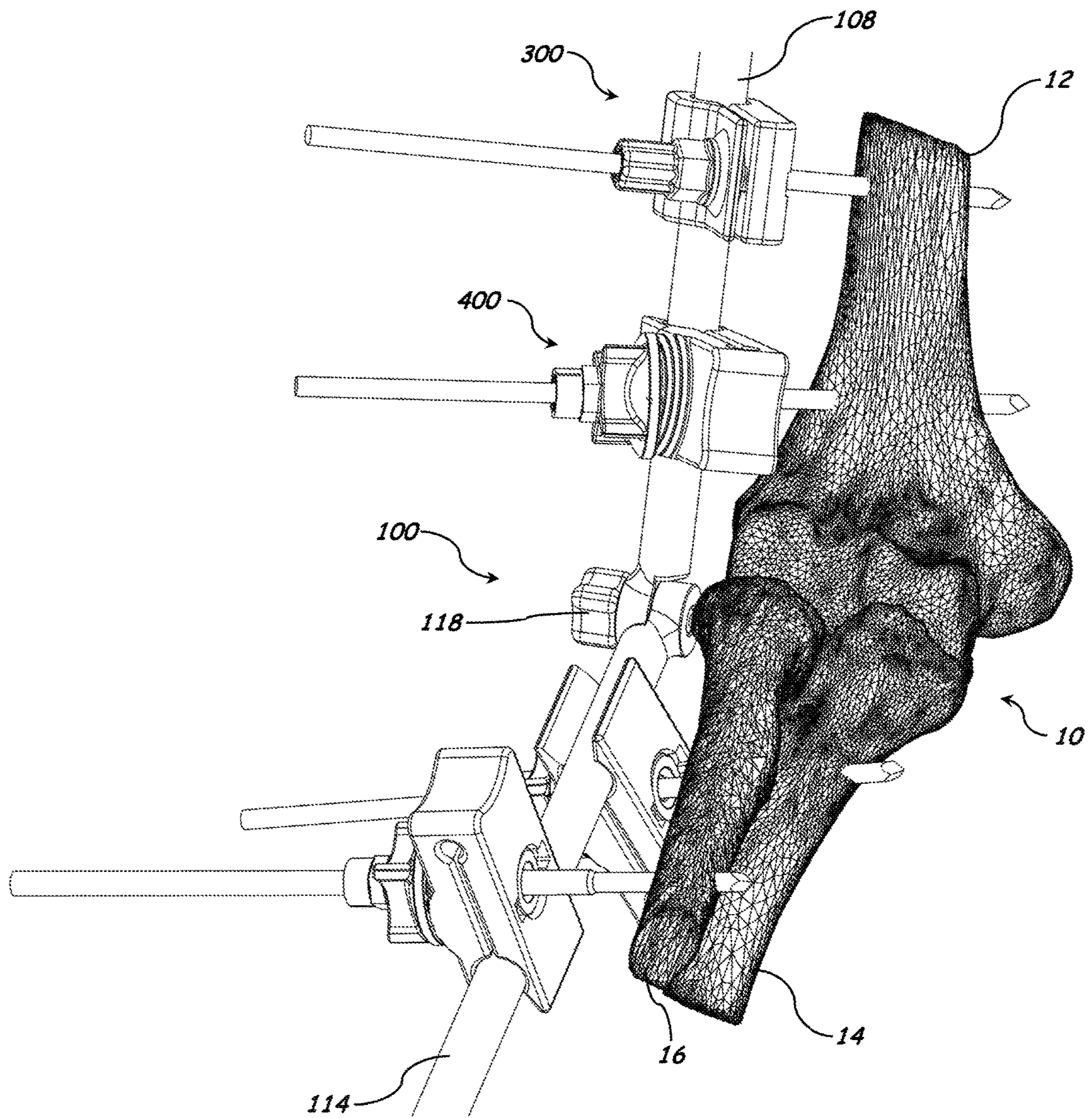


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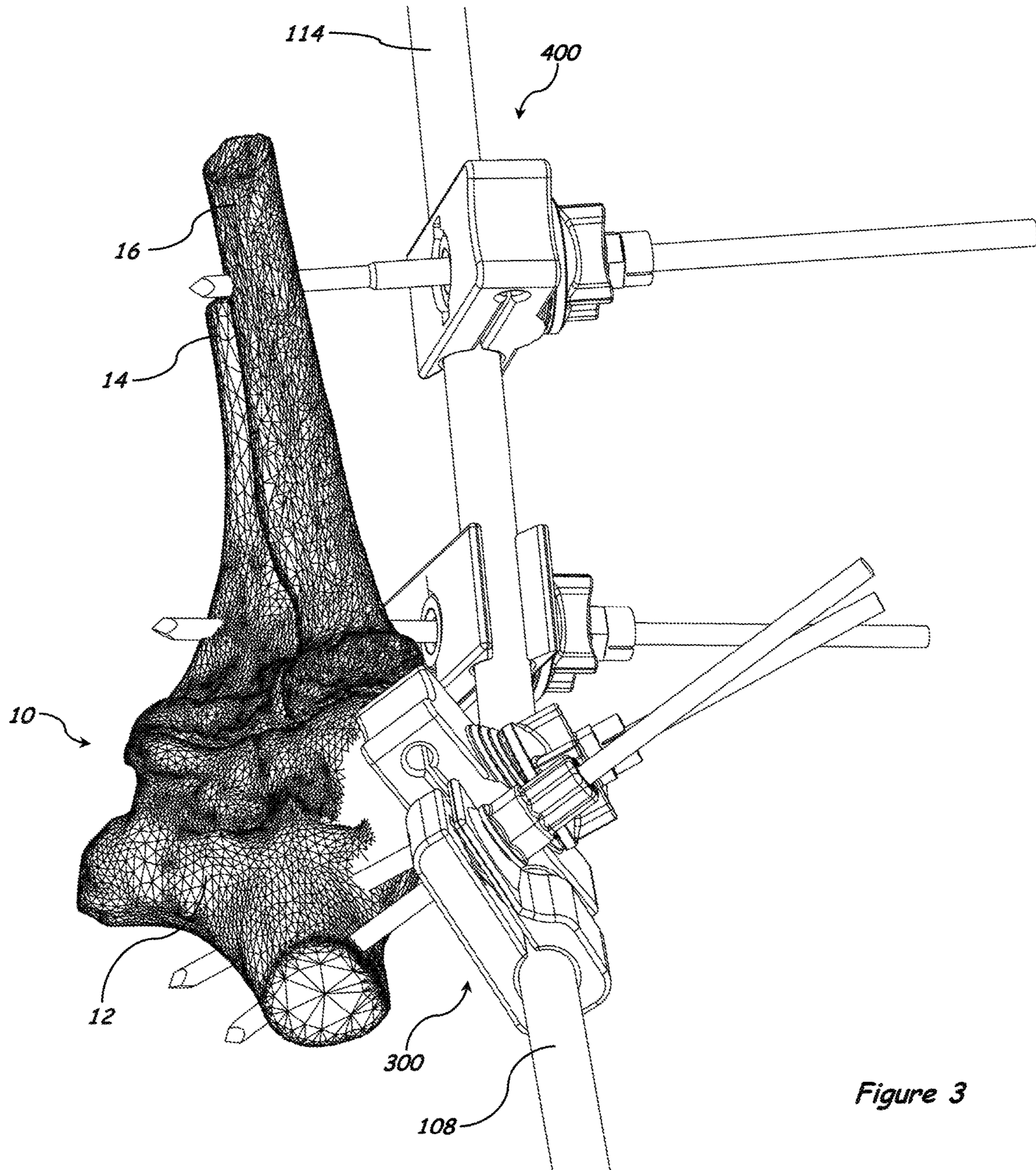
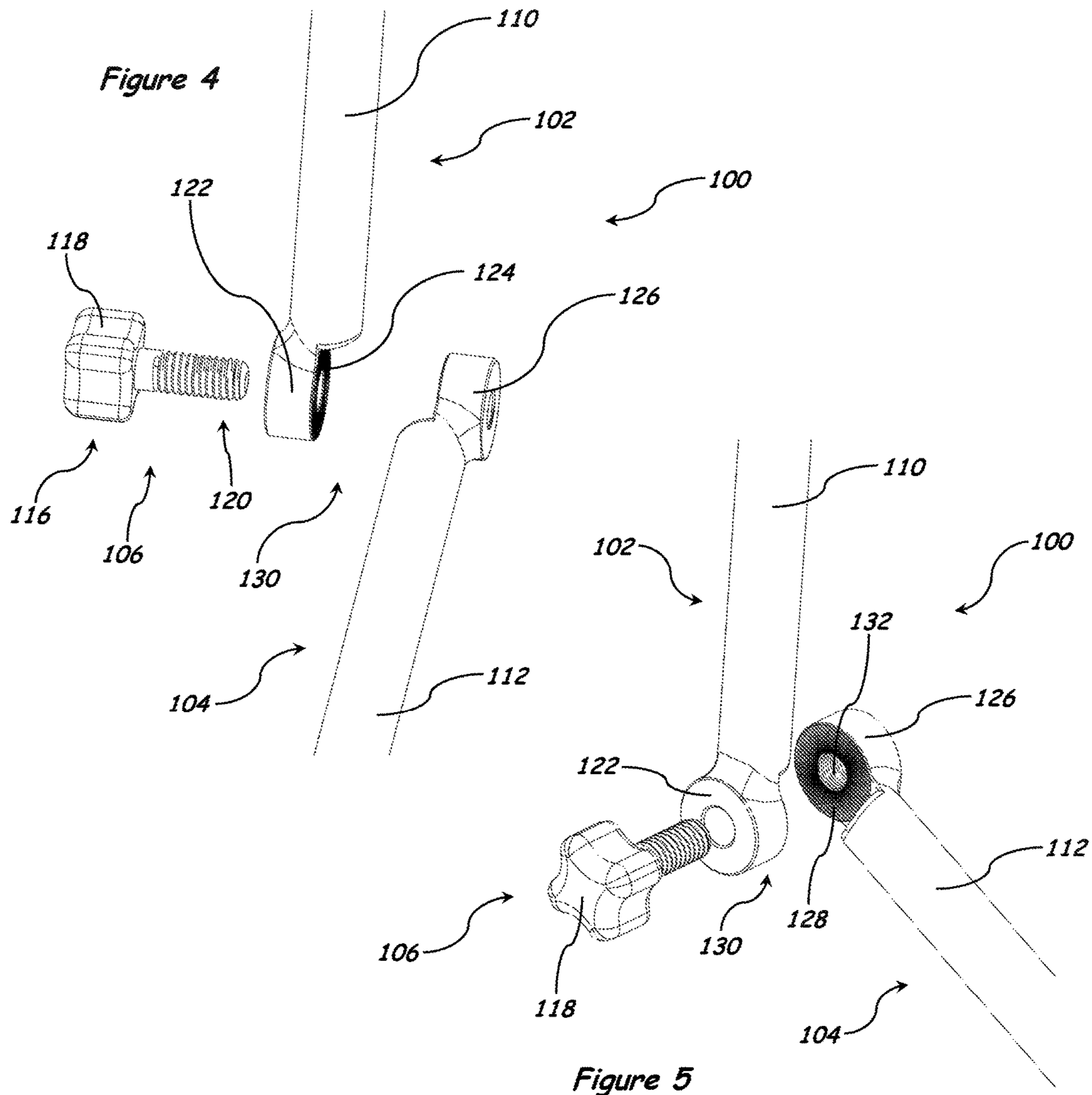
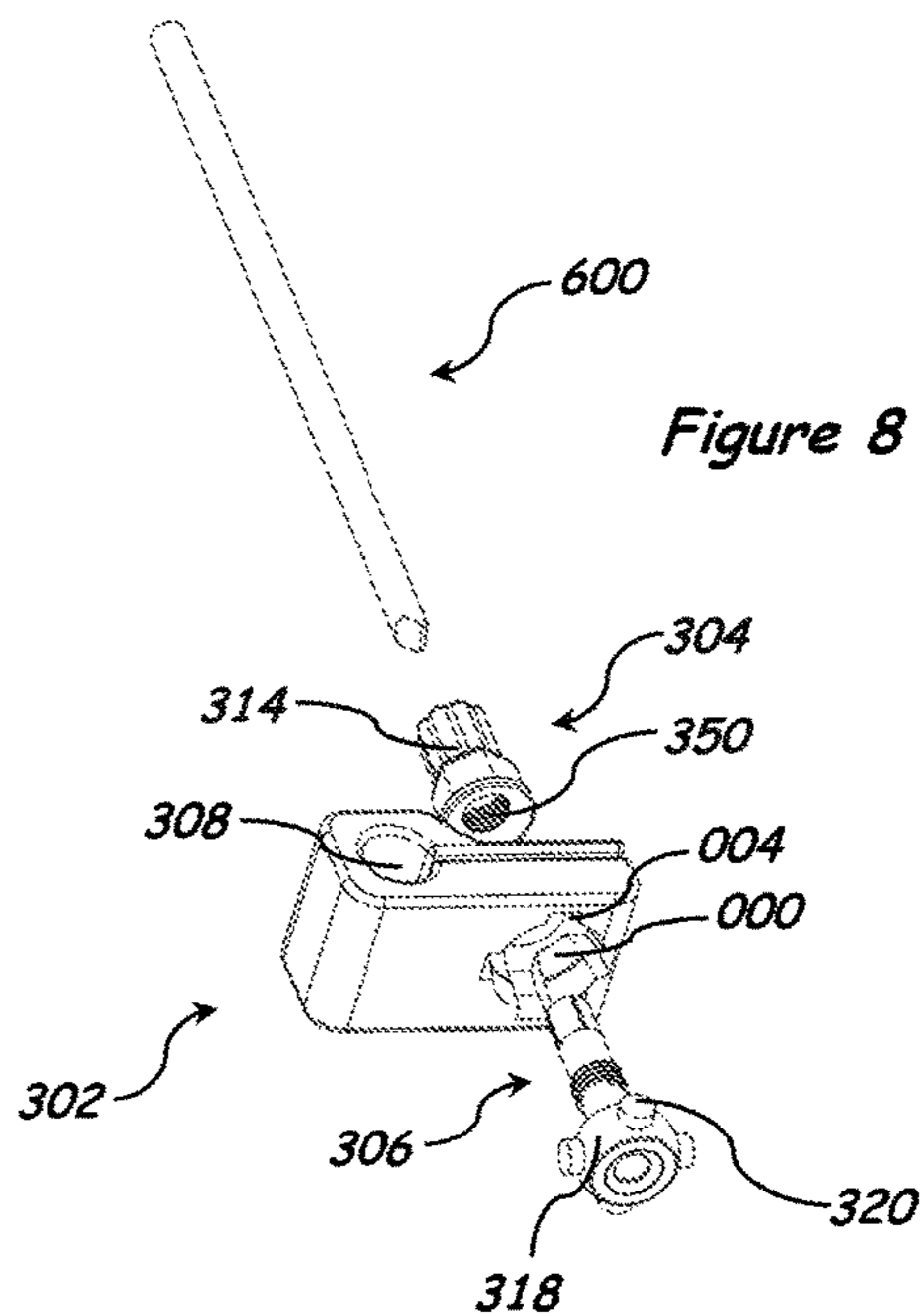
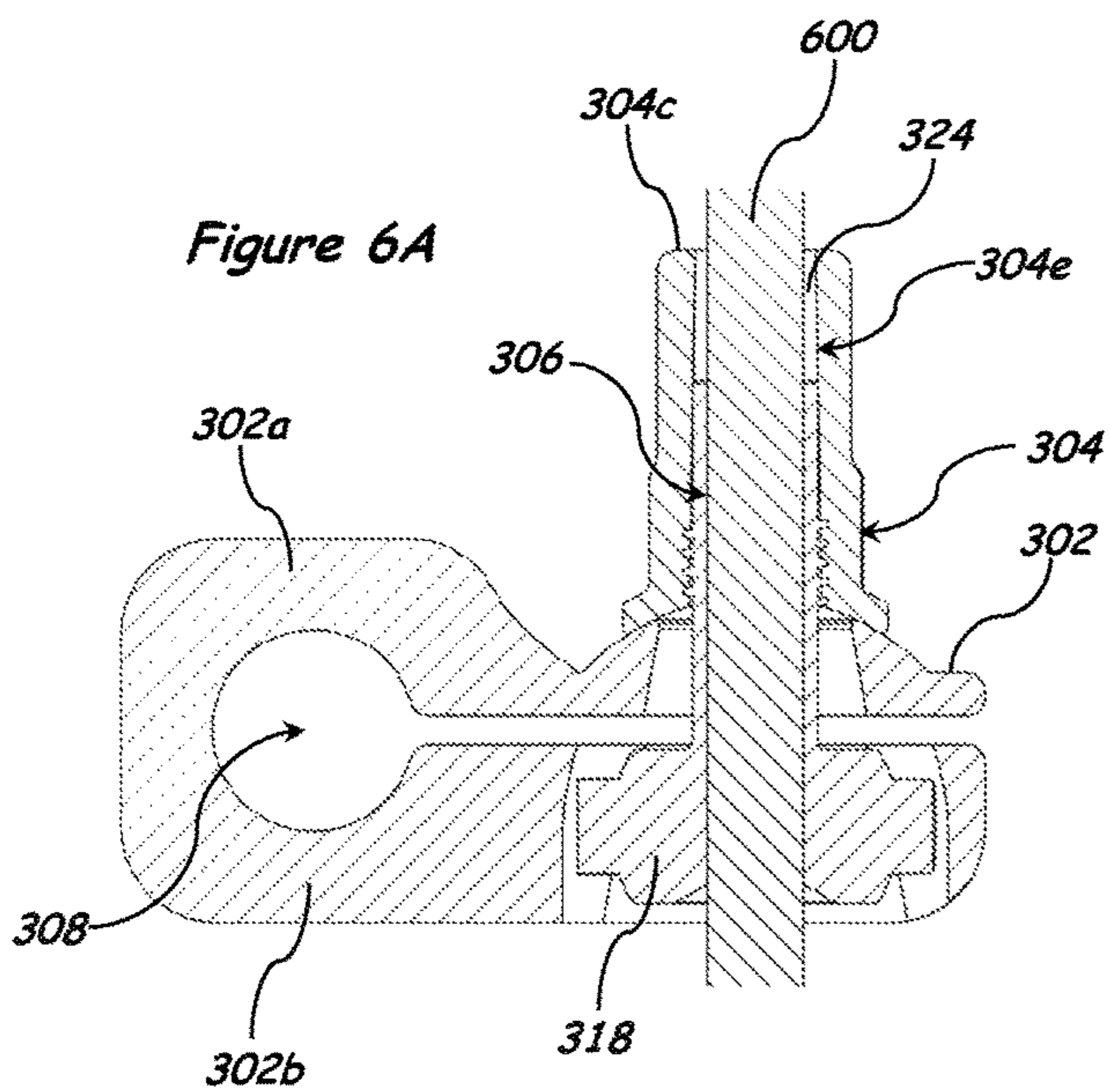
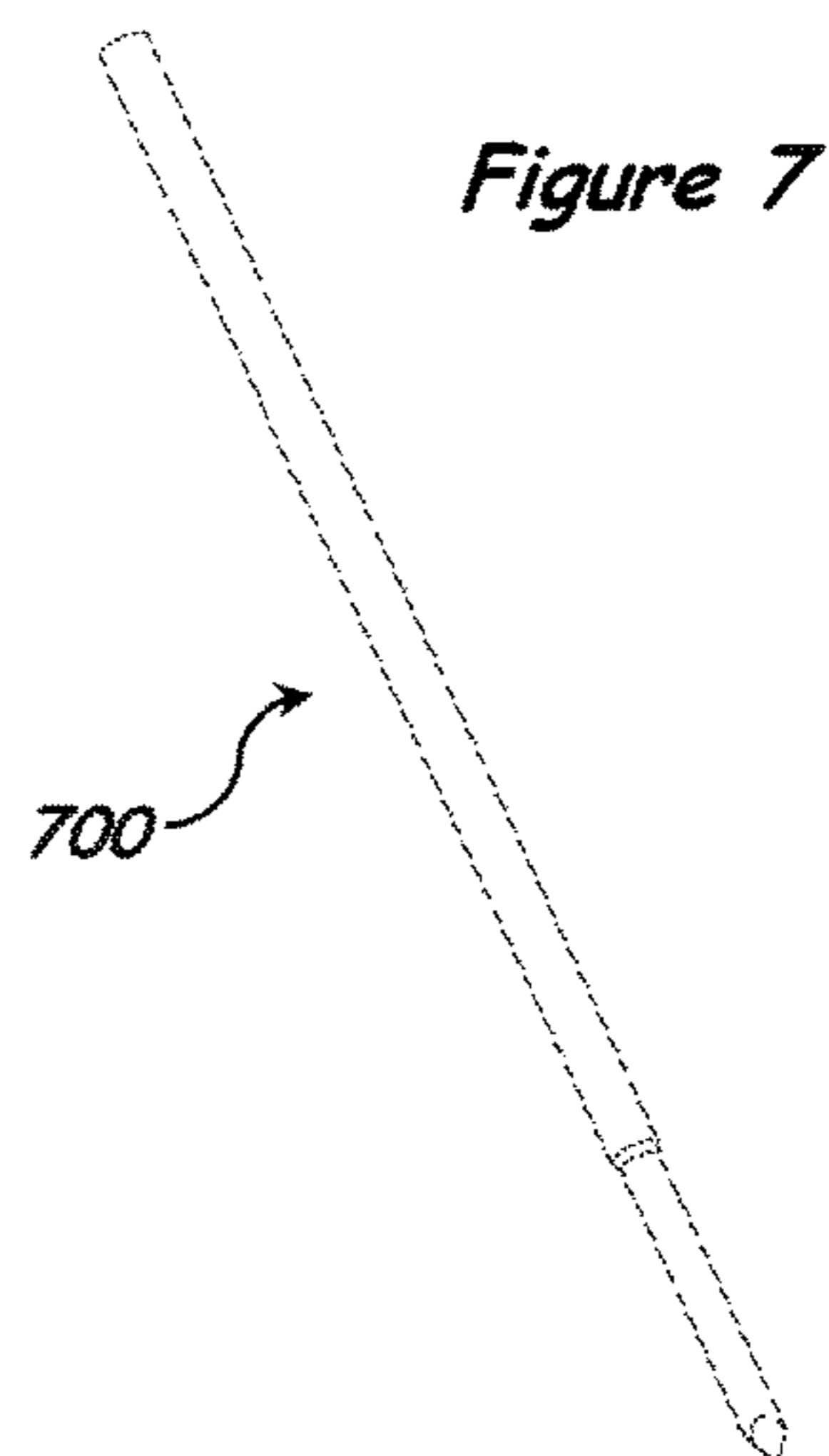
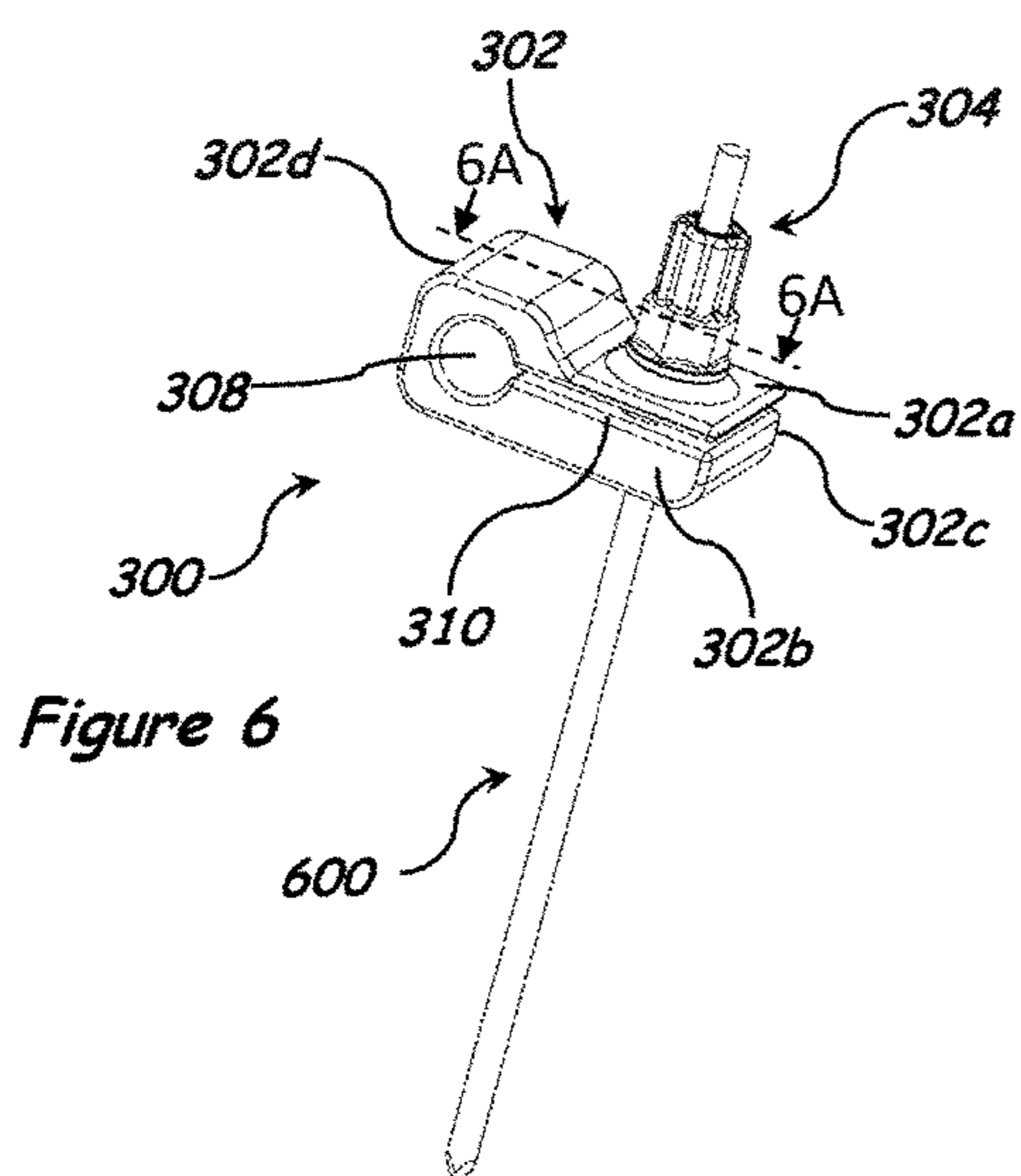


Figure 3





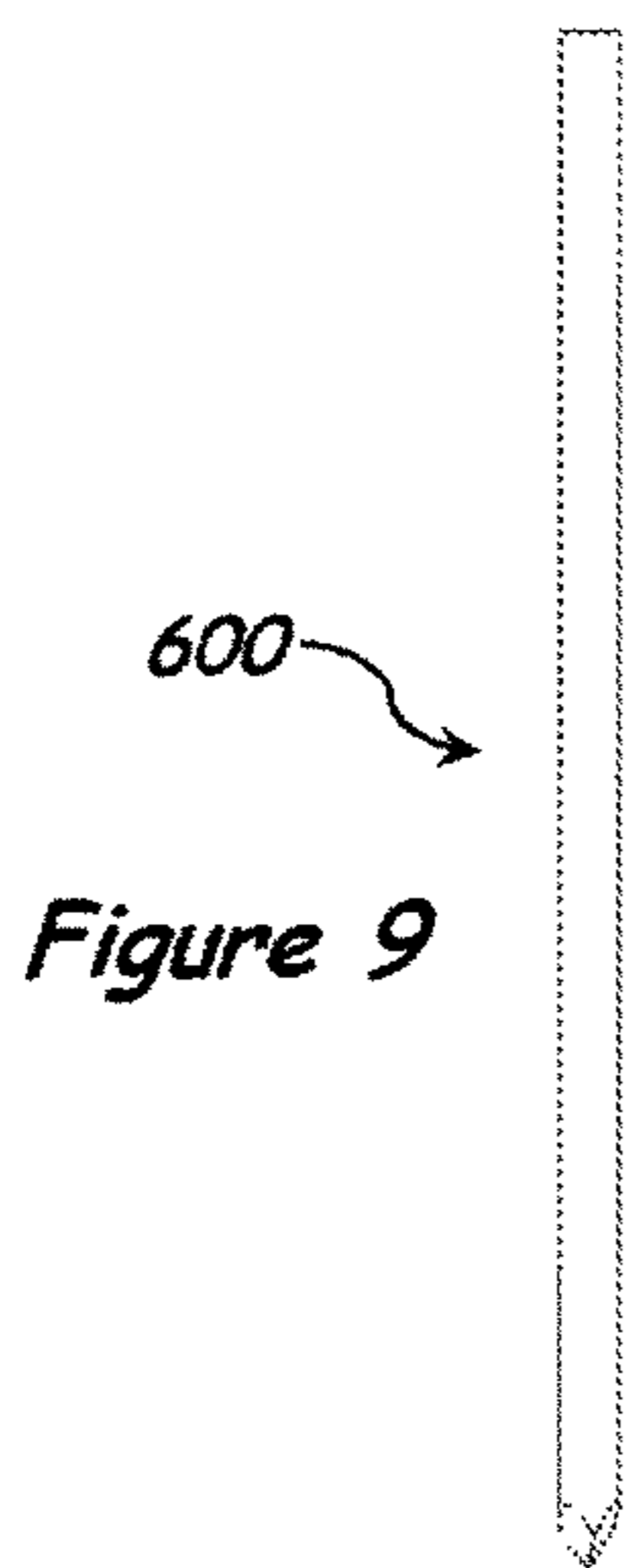


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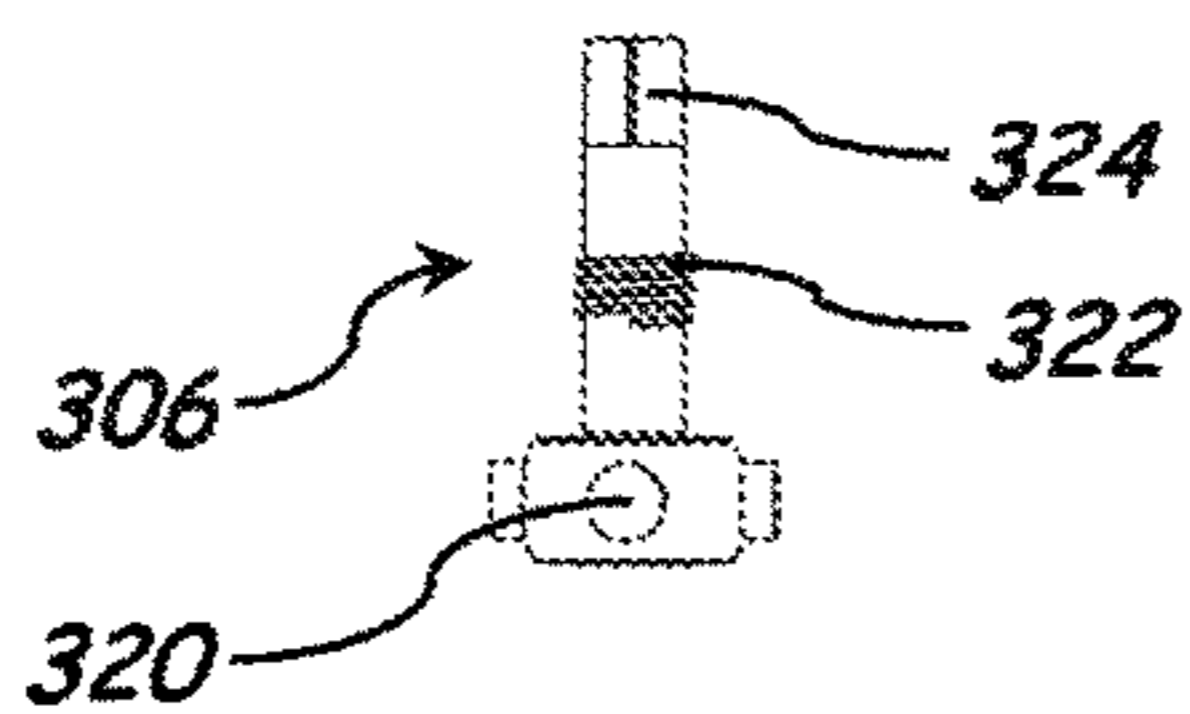
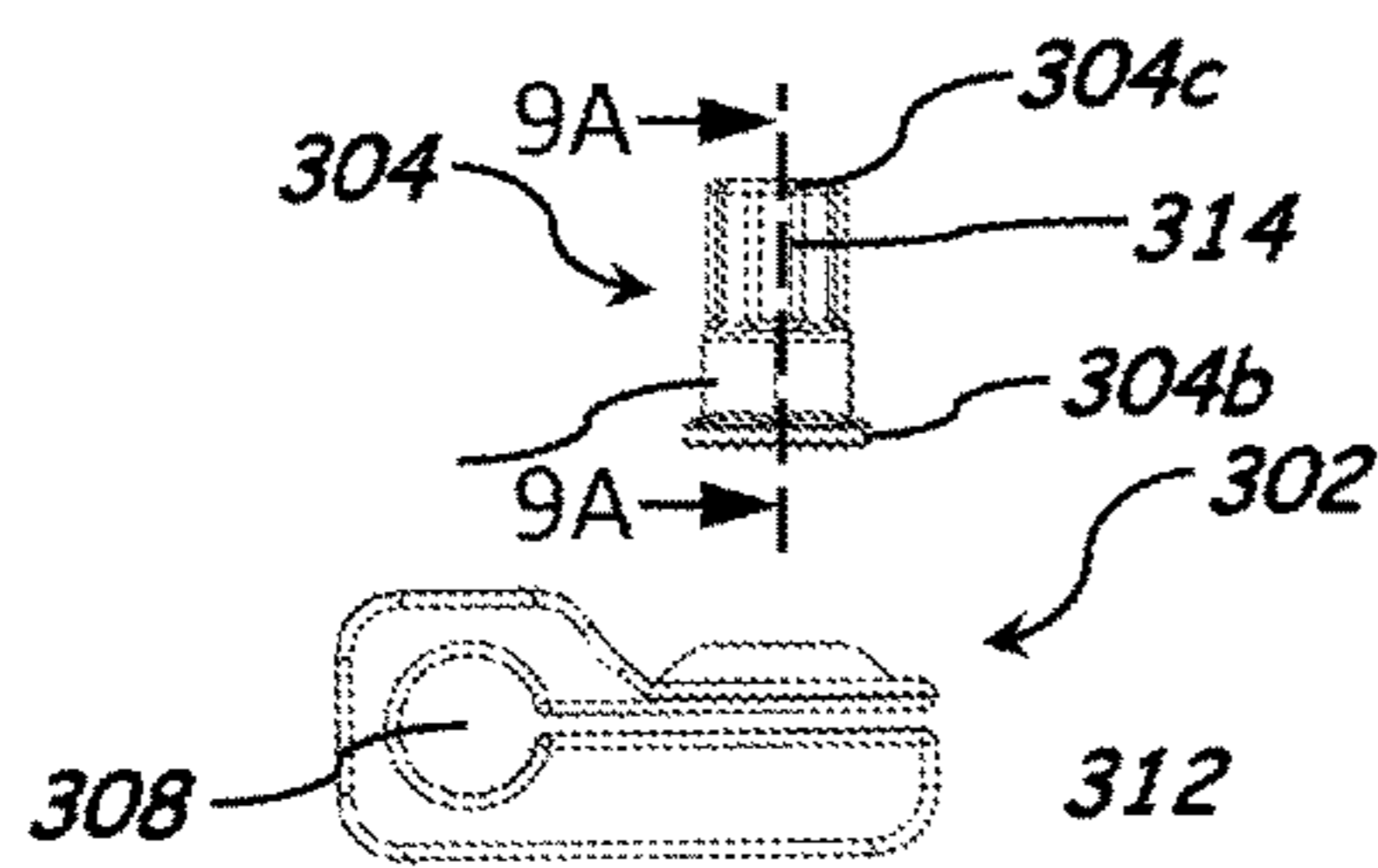


Figure 9A

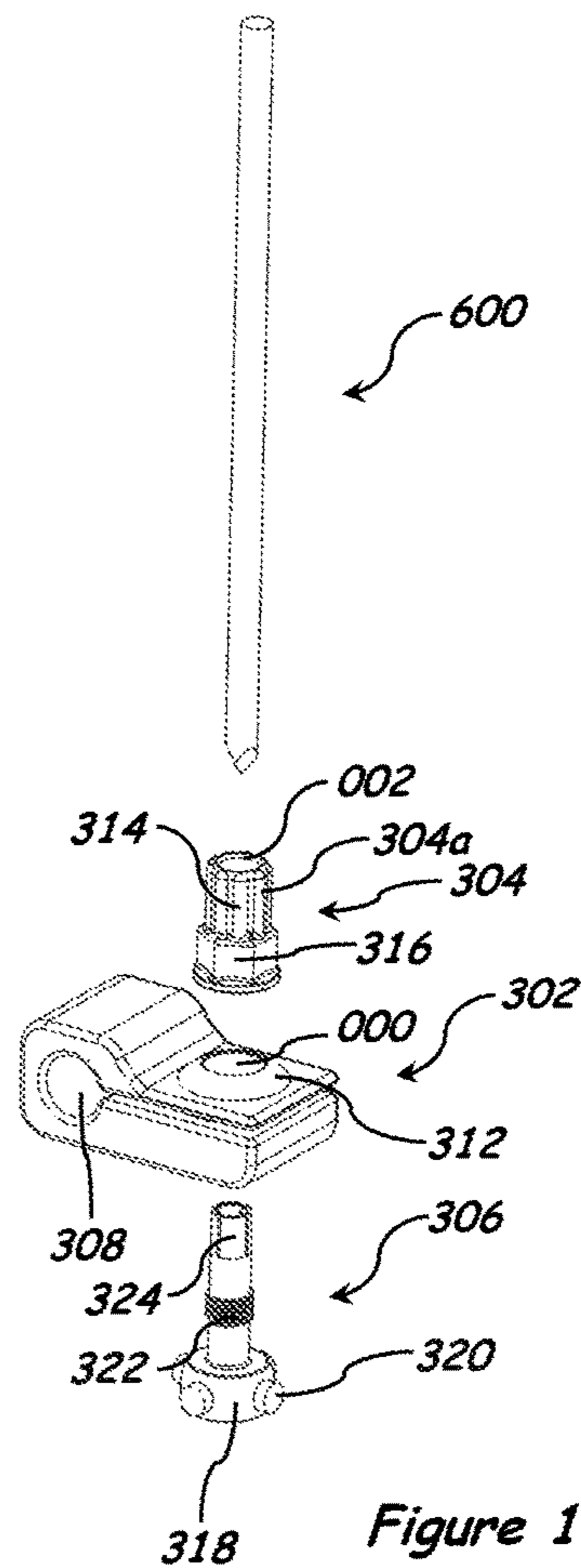
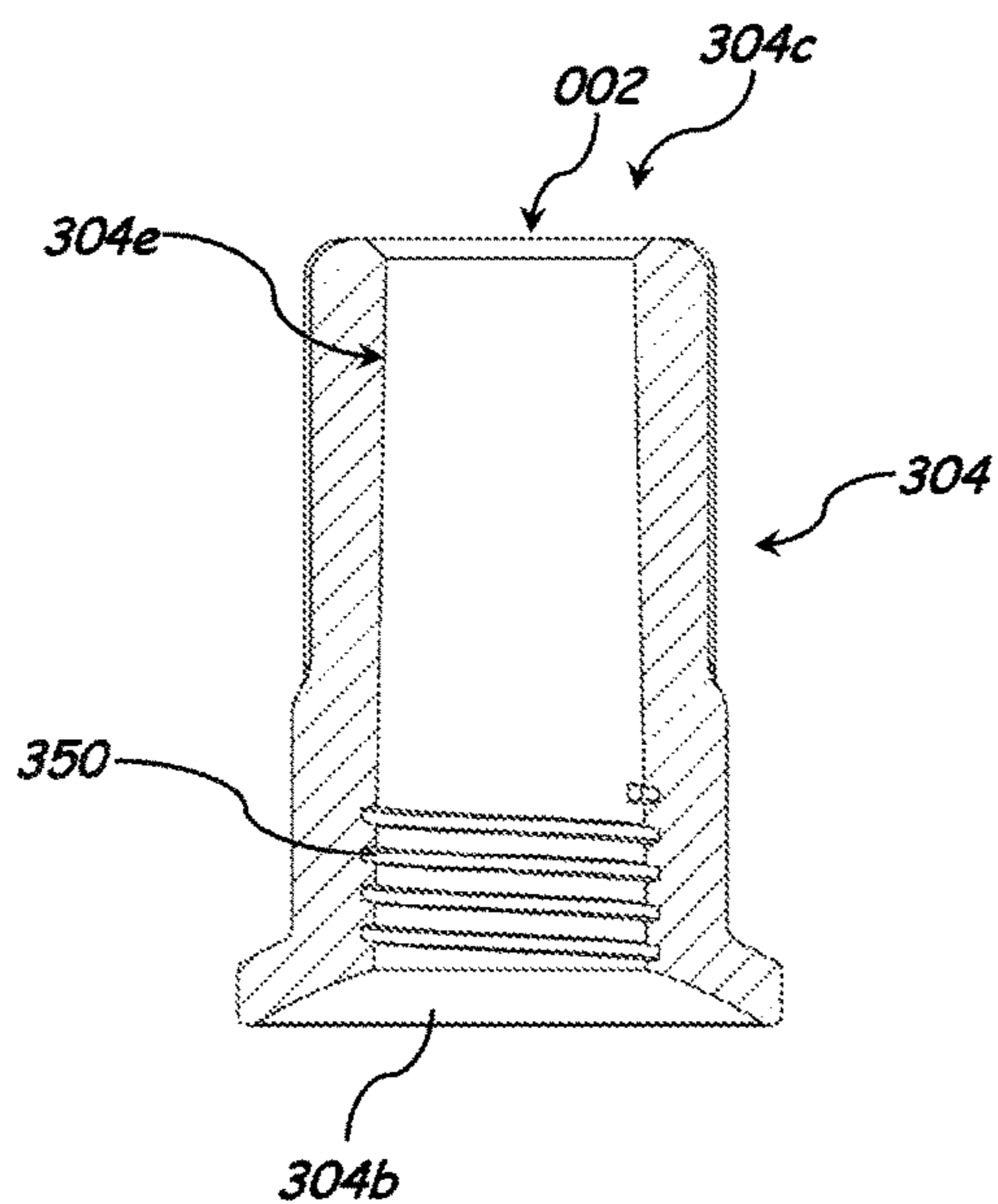
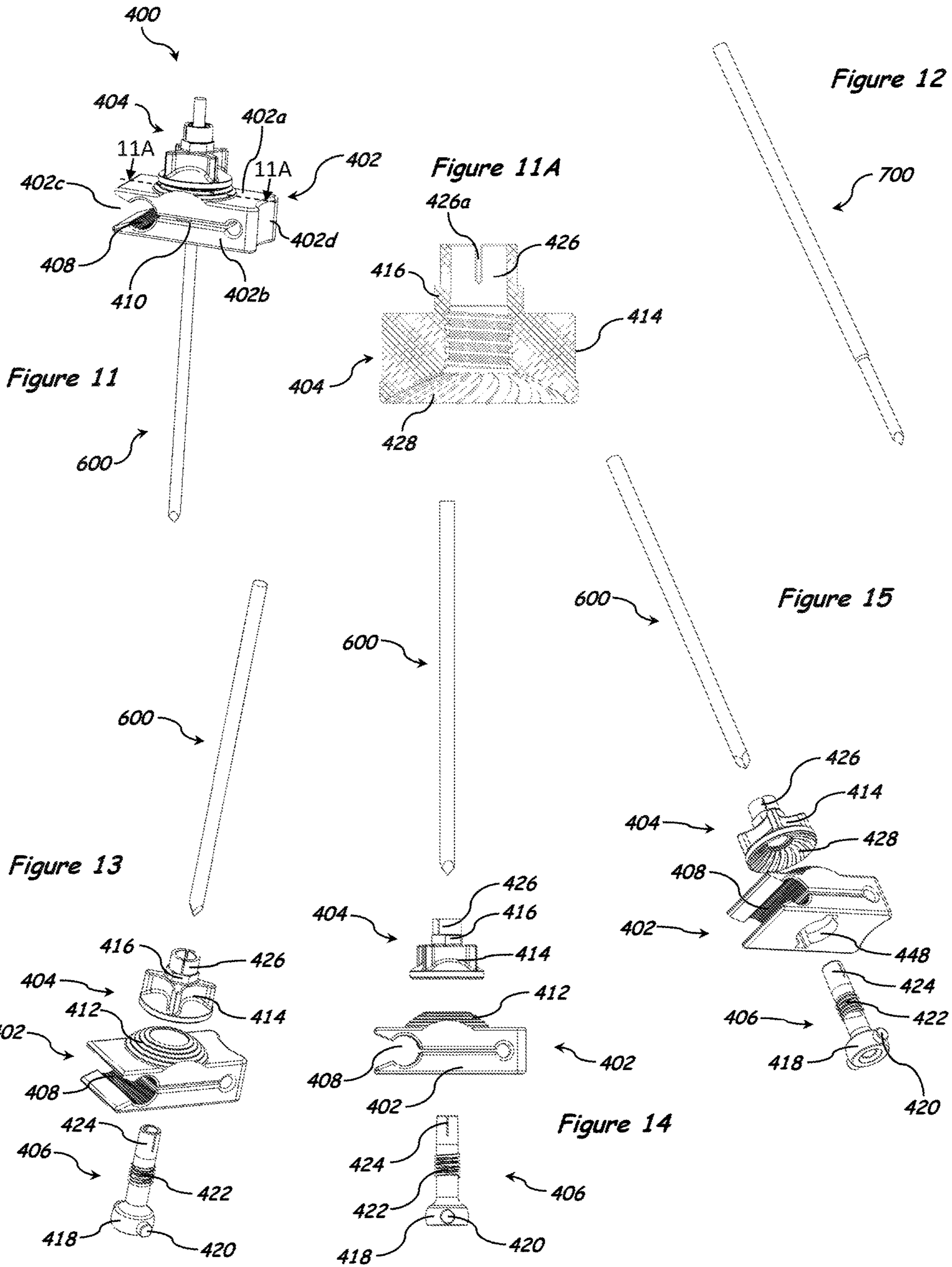
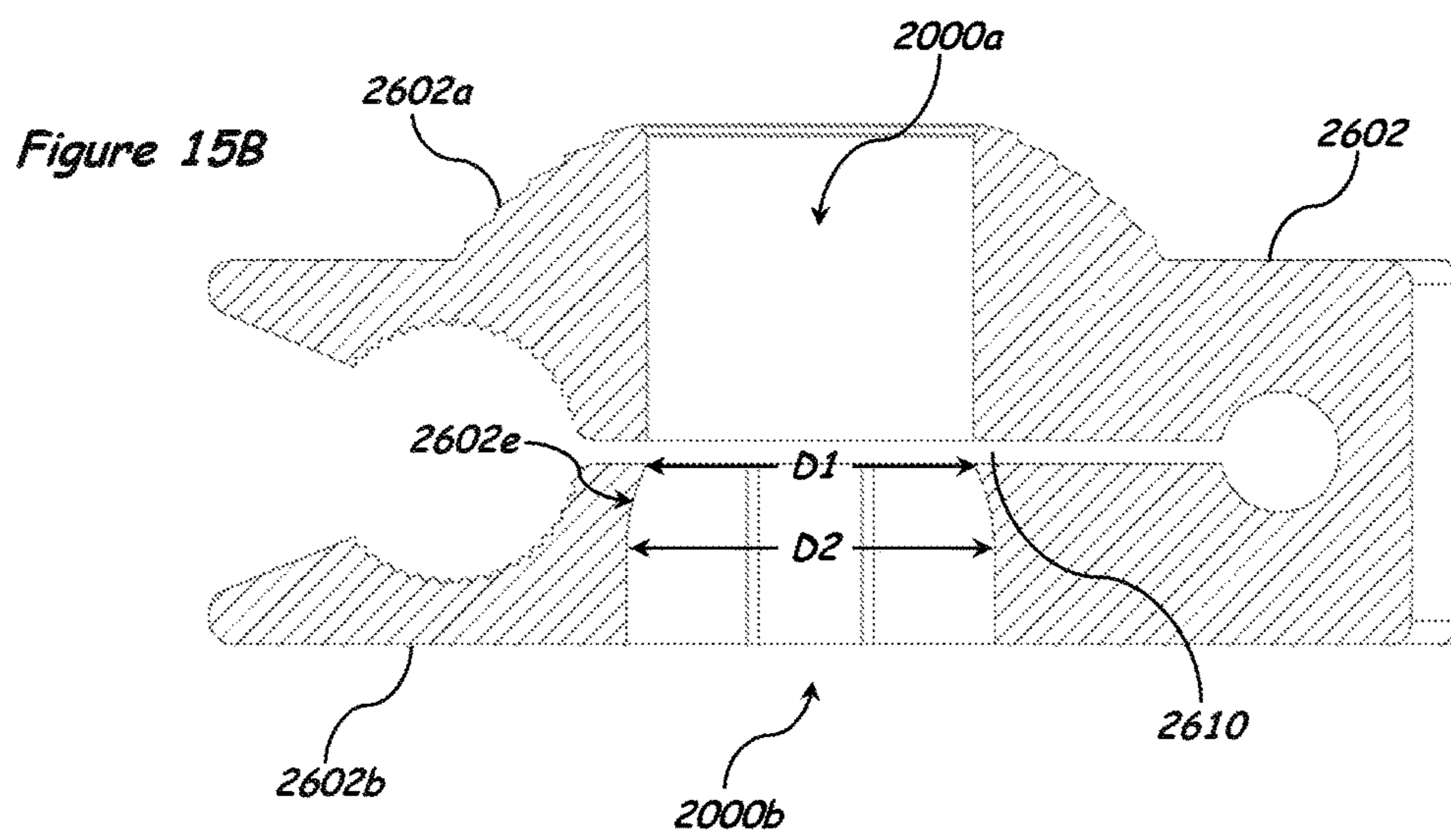
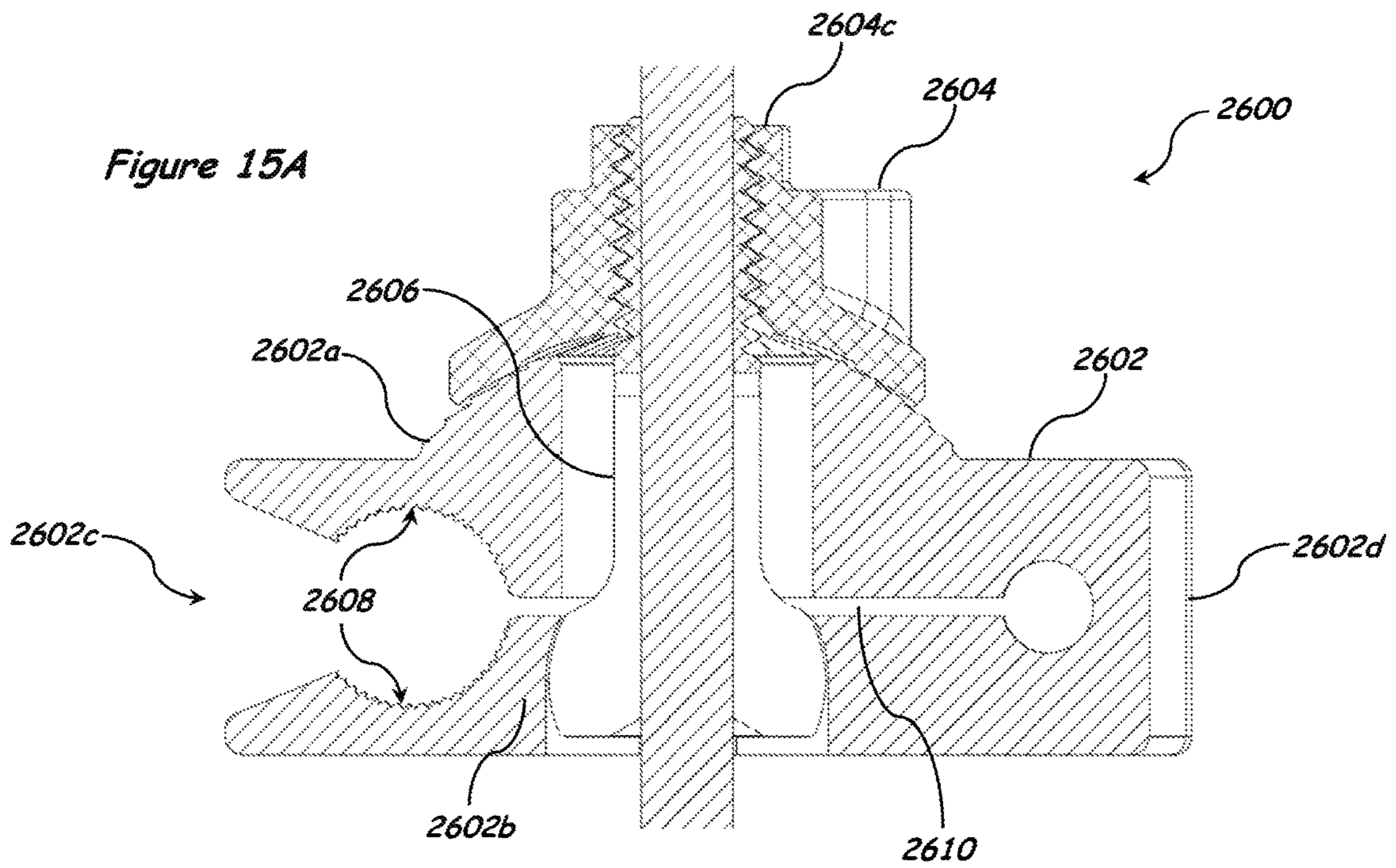


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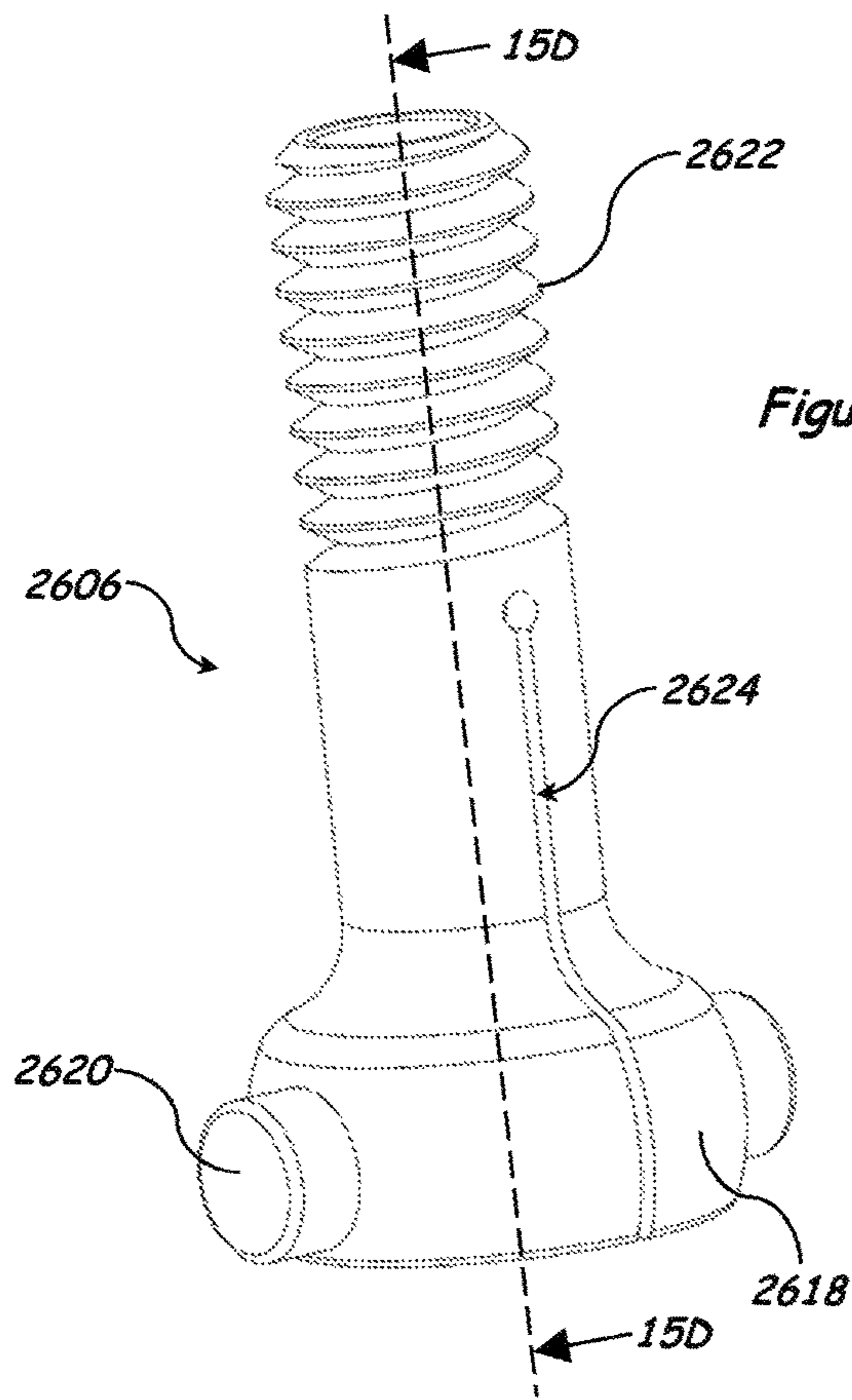


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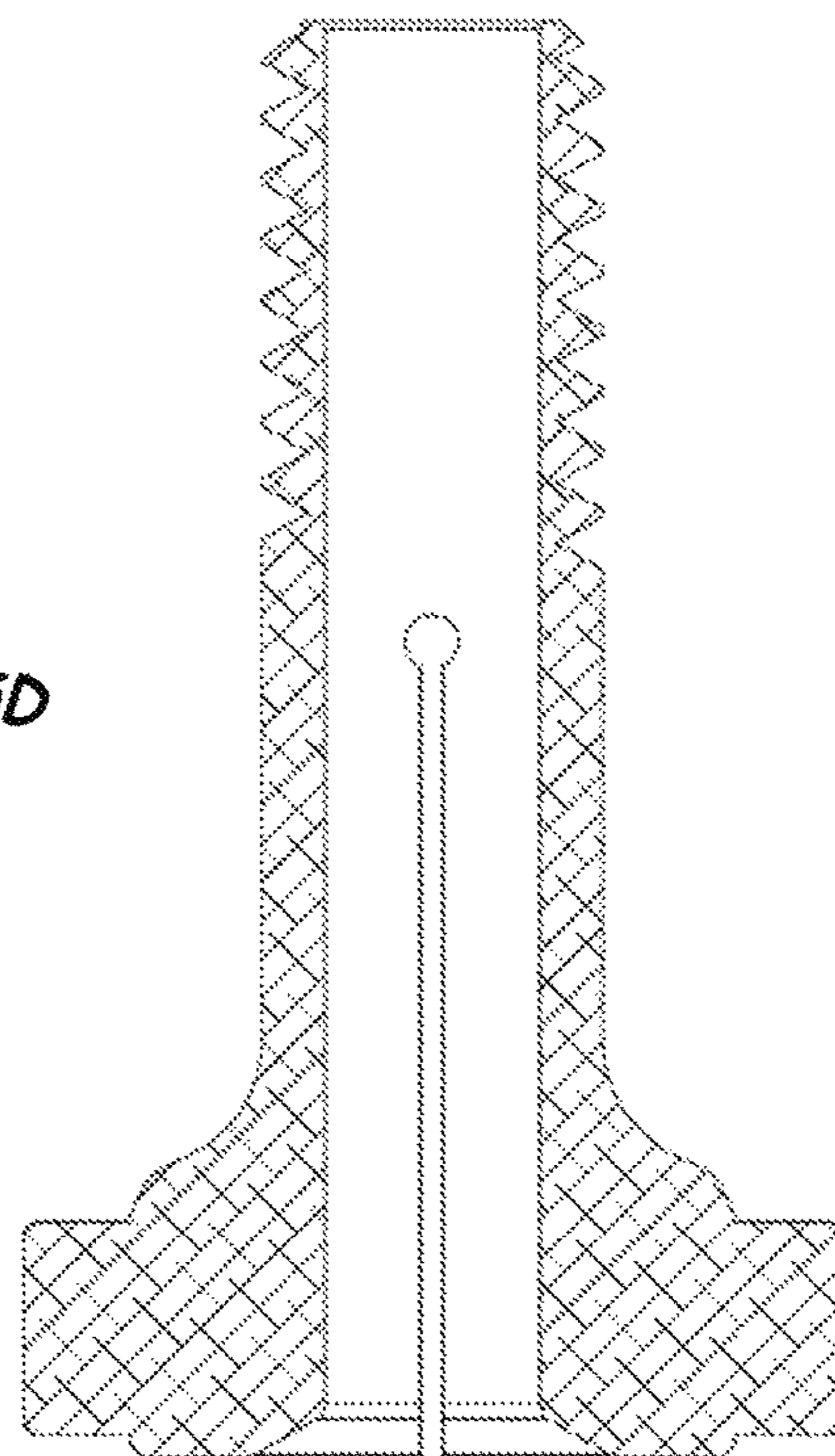
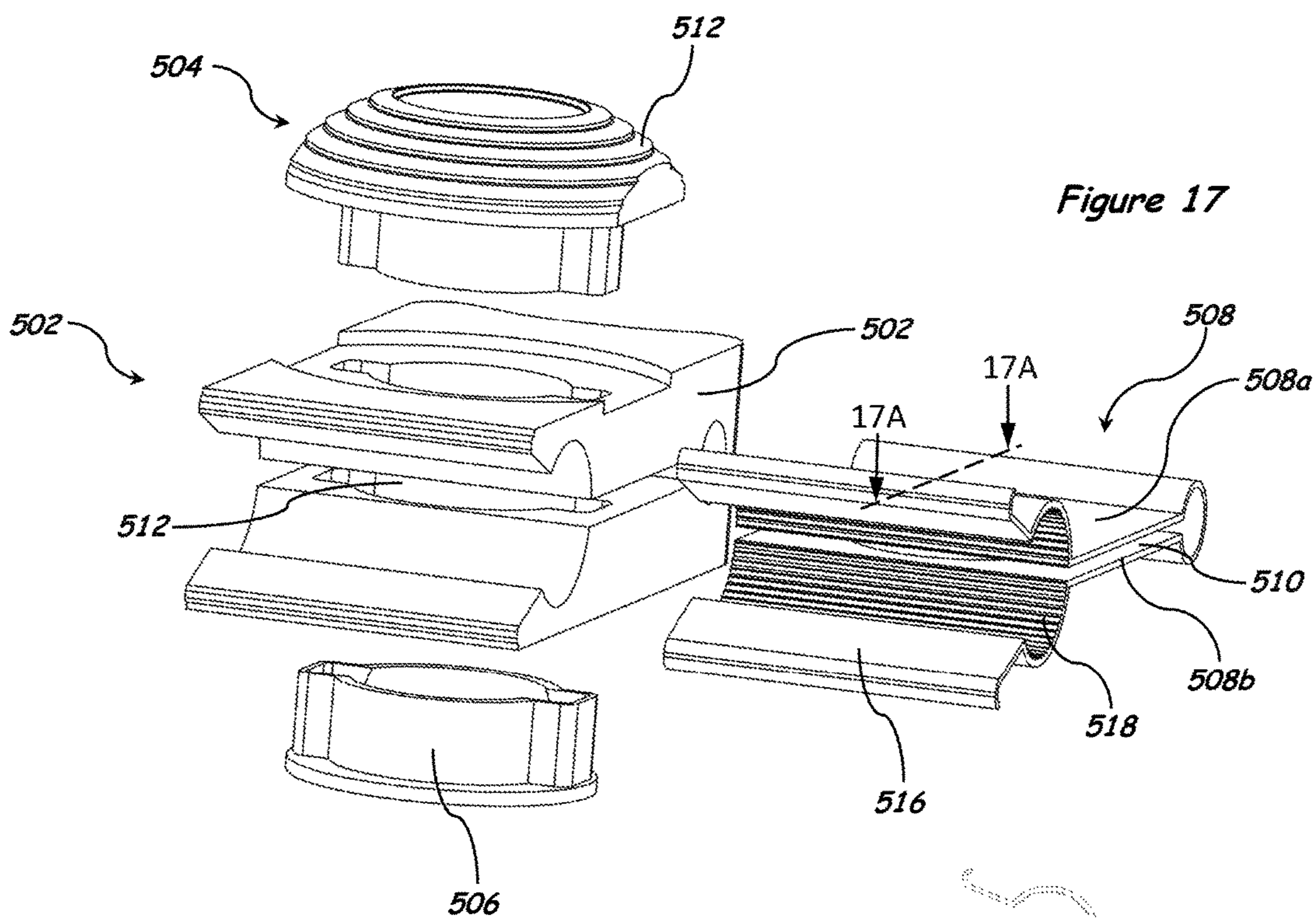
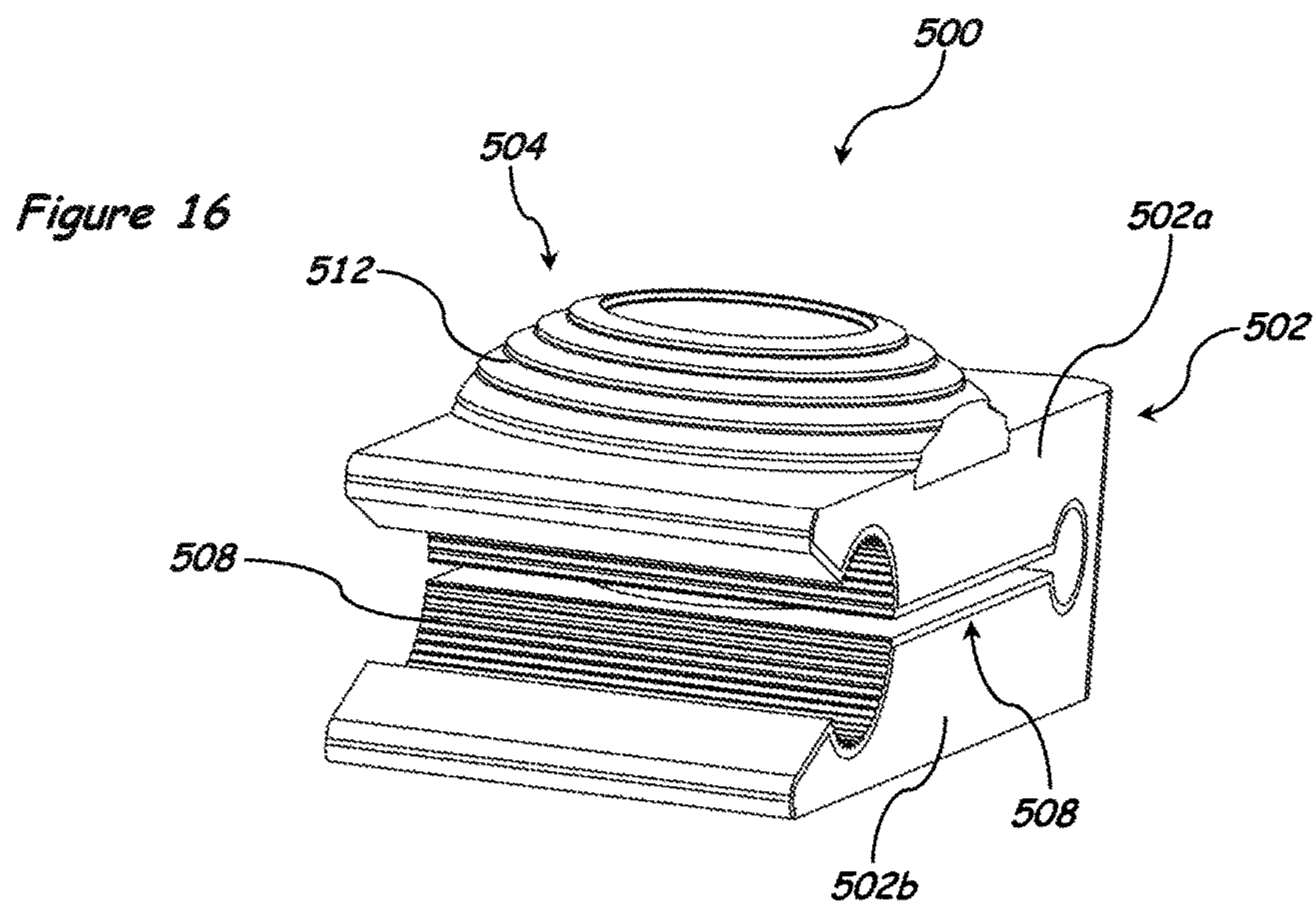
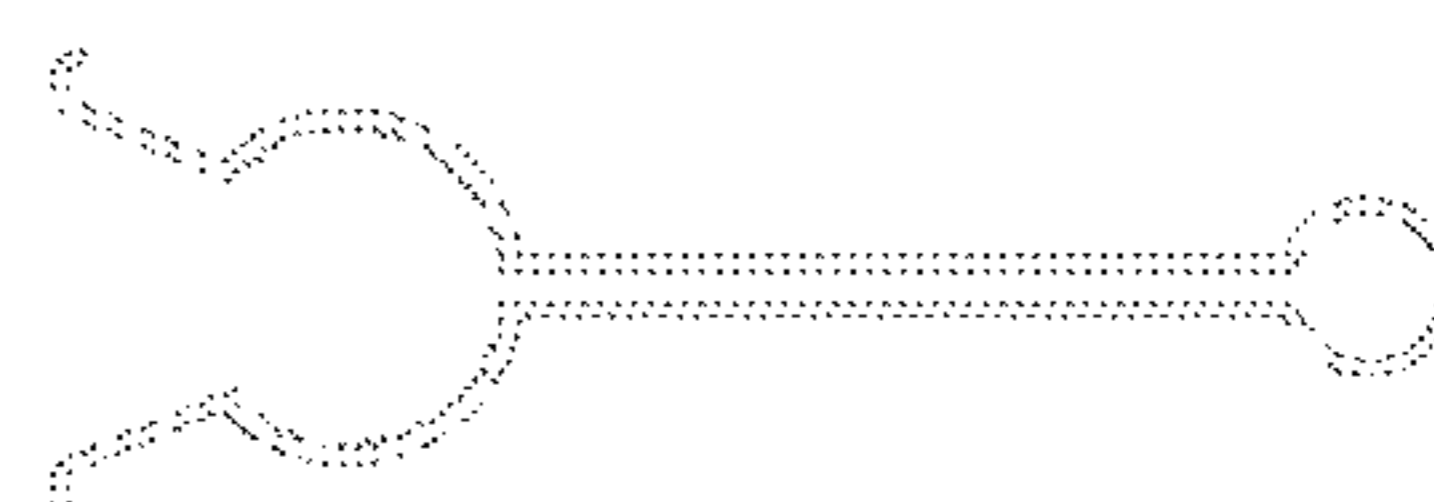
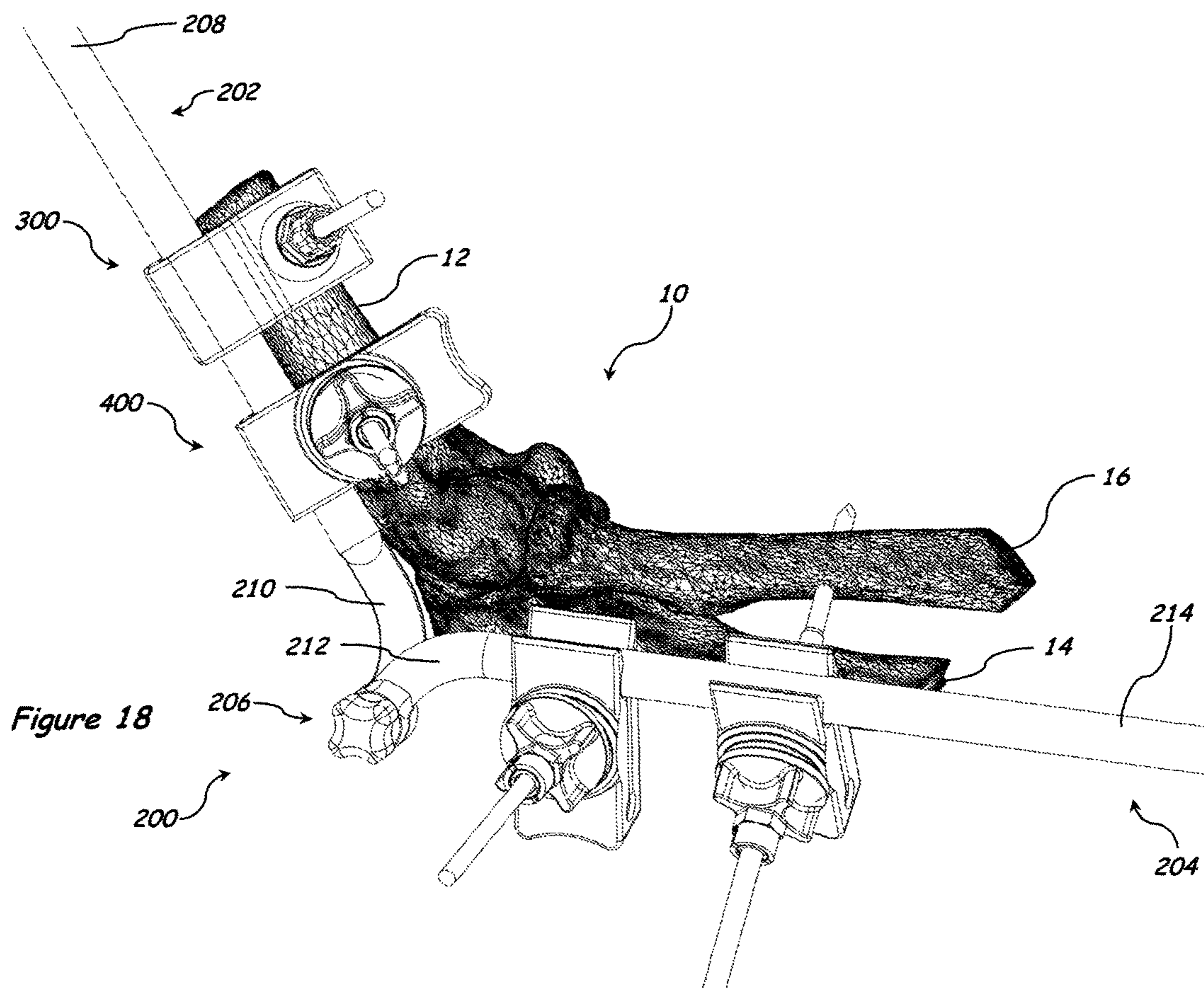


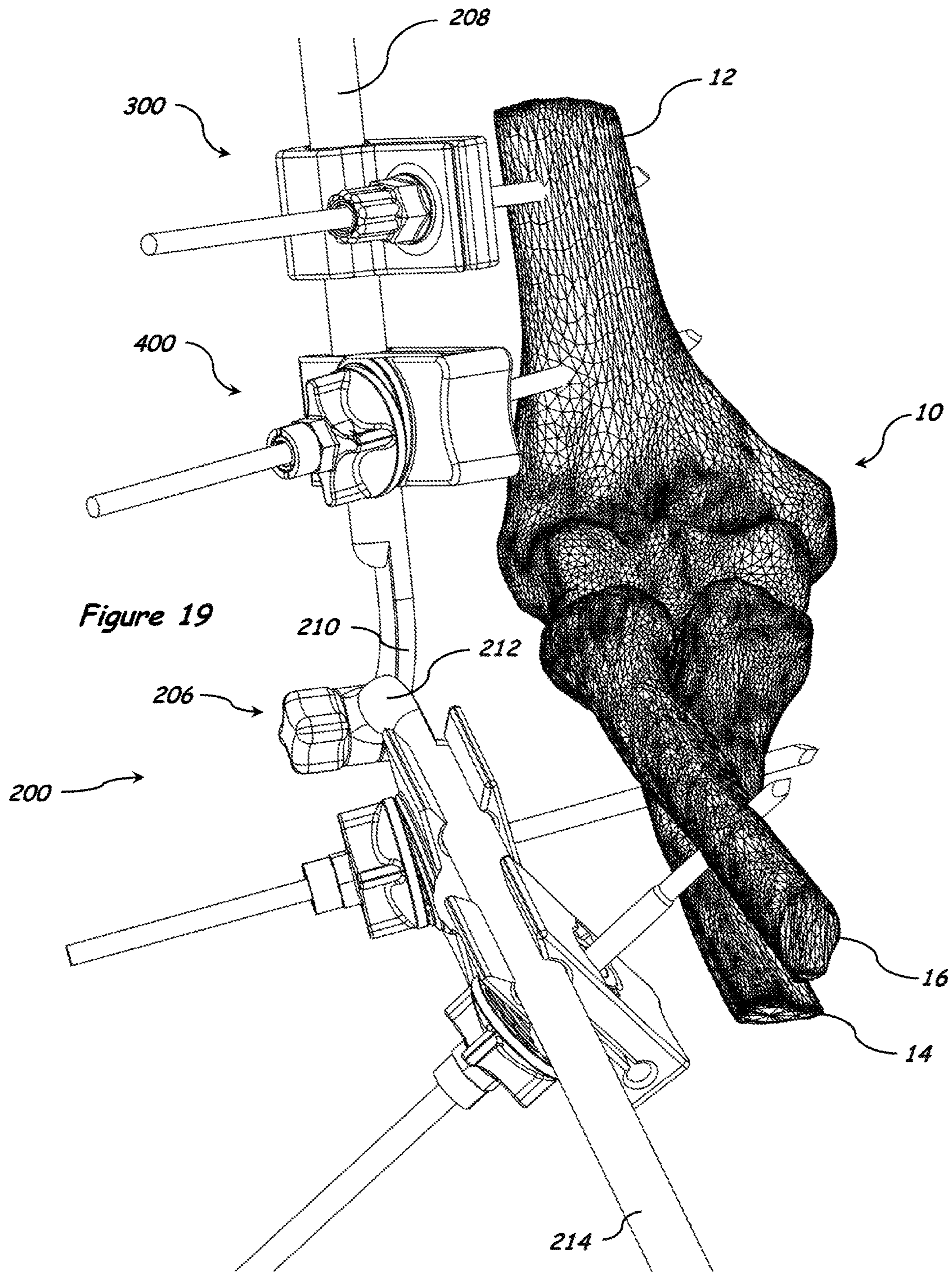
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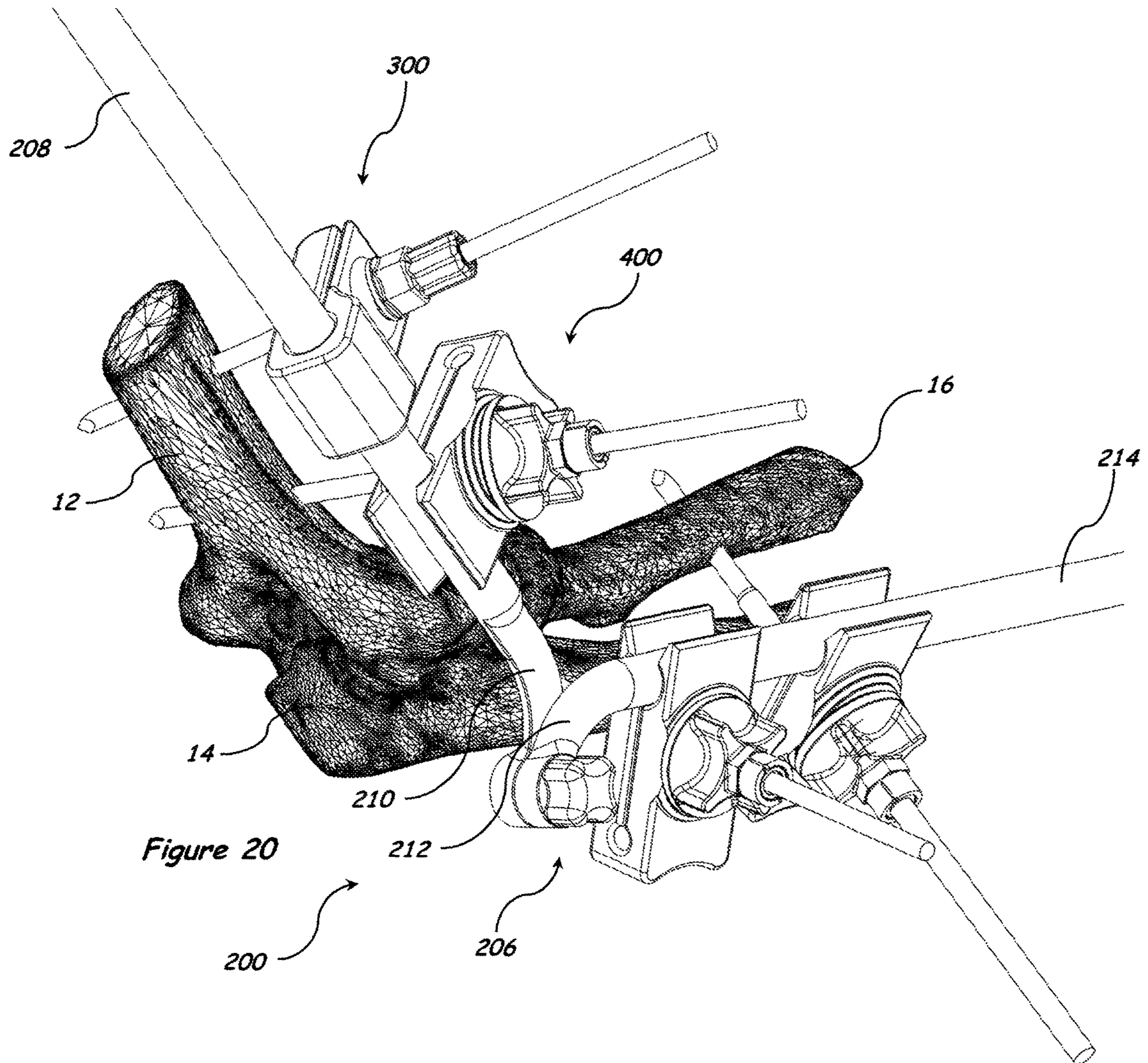


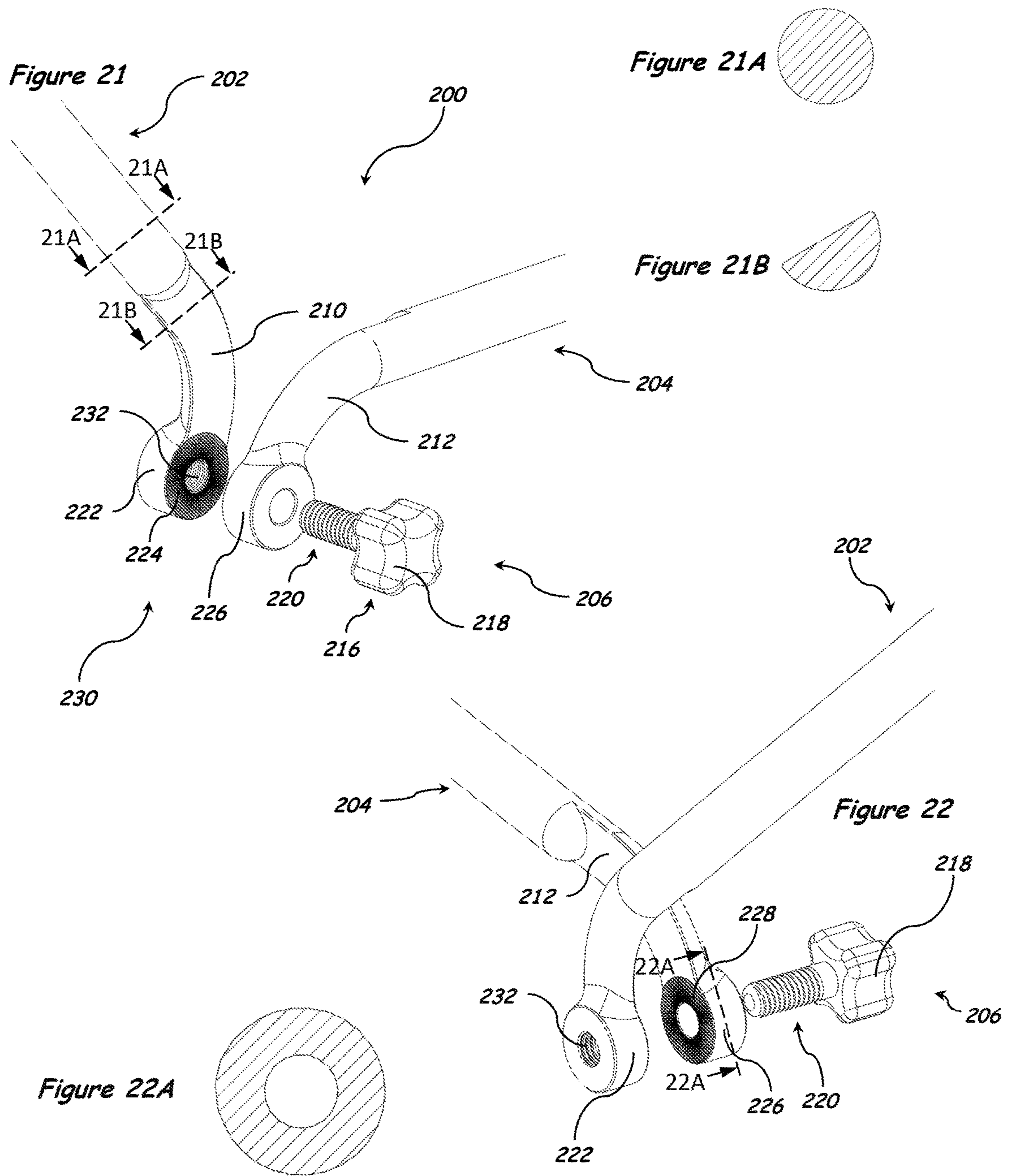
*Figure 17A*













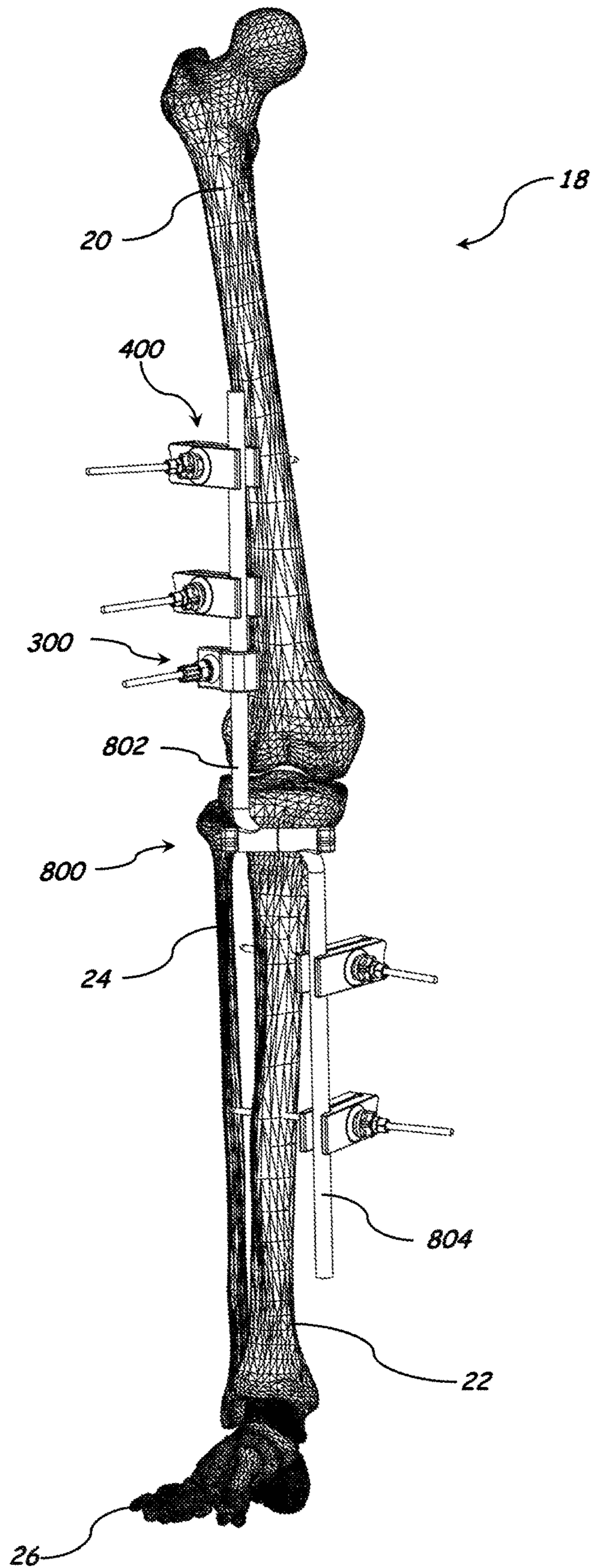


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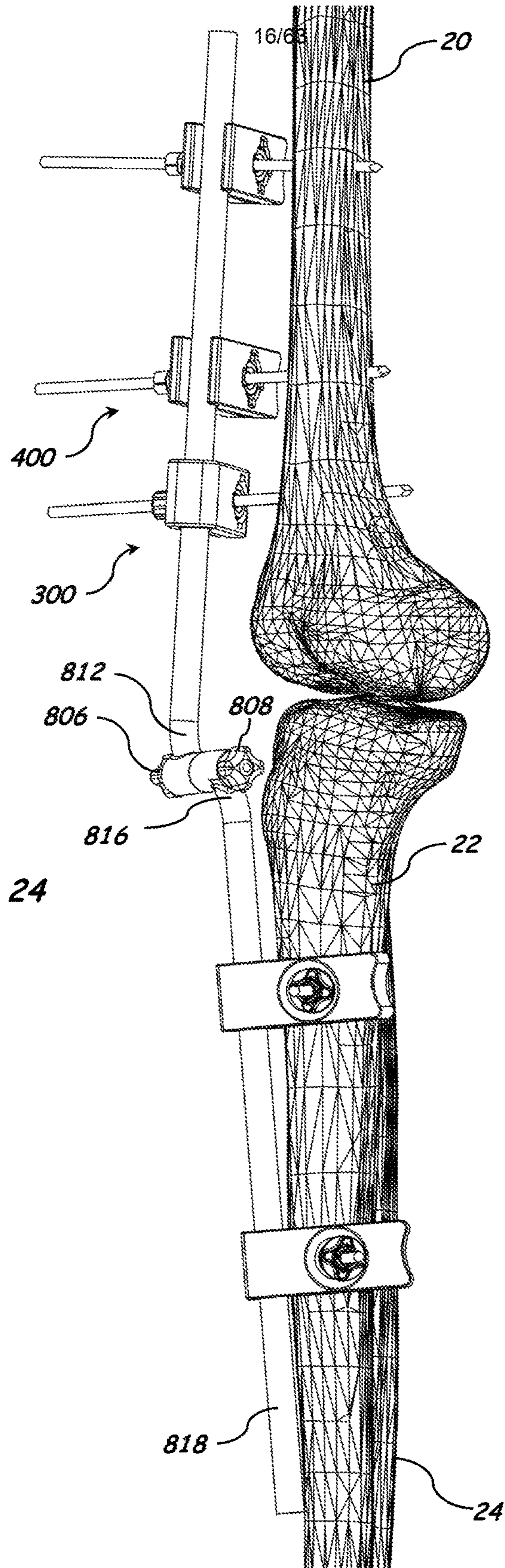
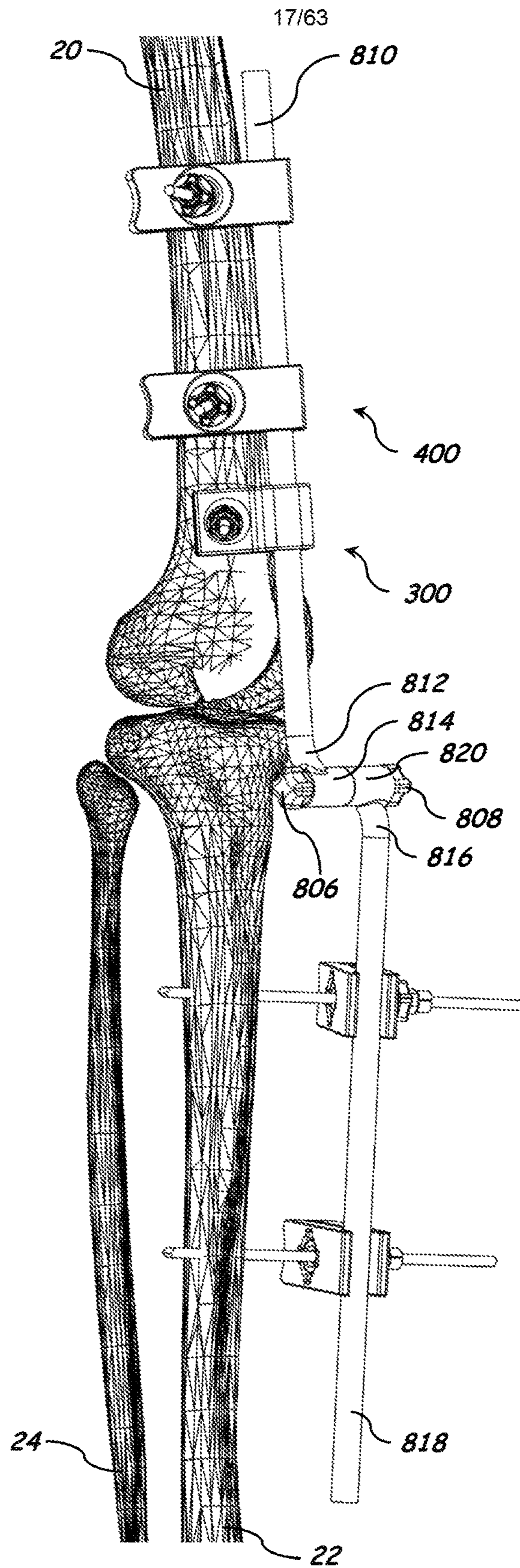
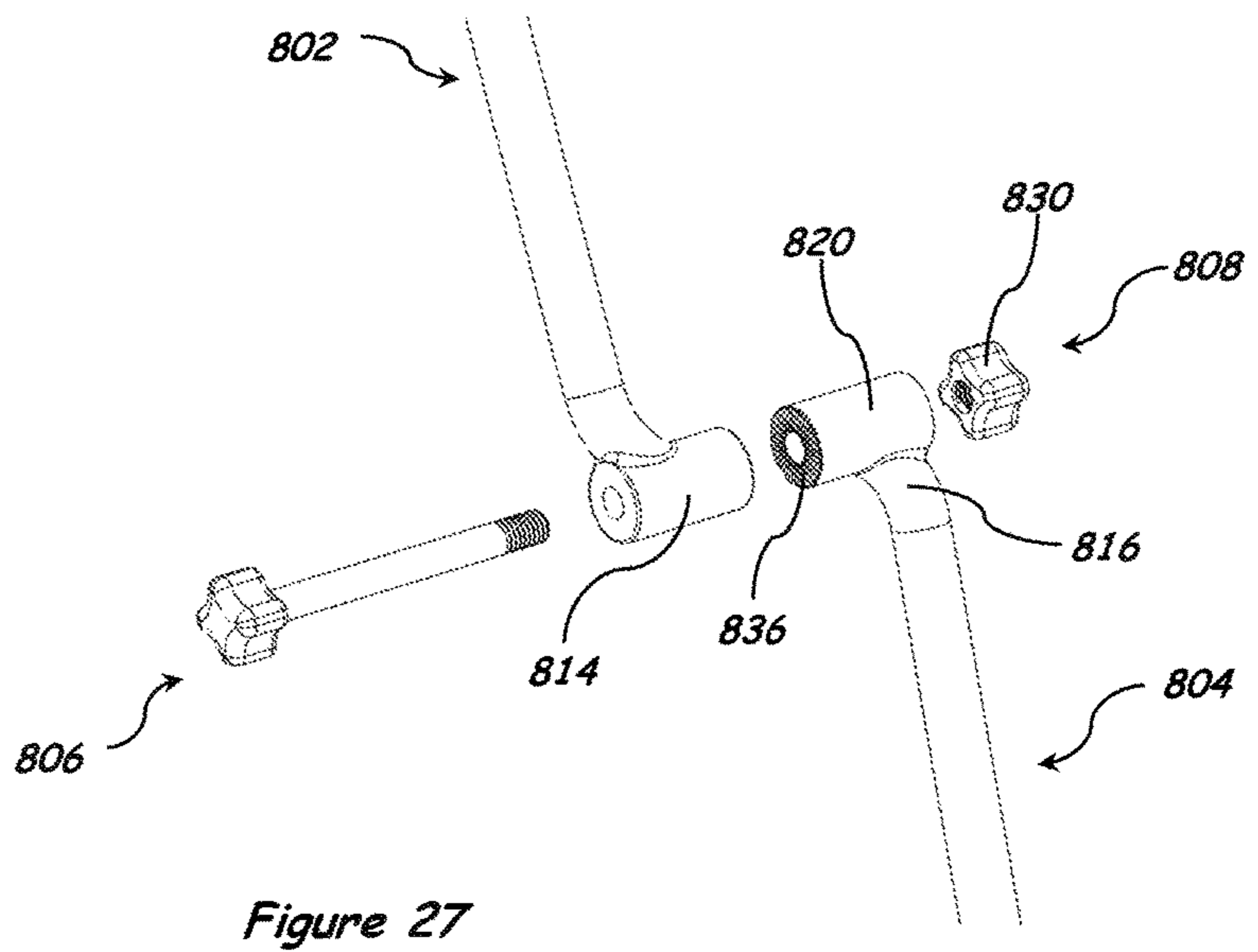
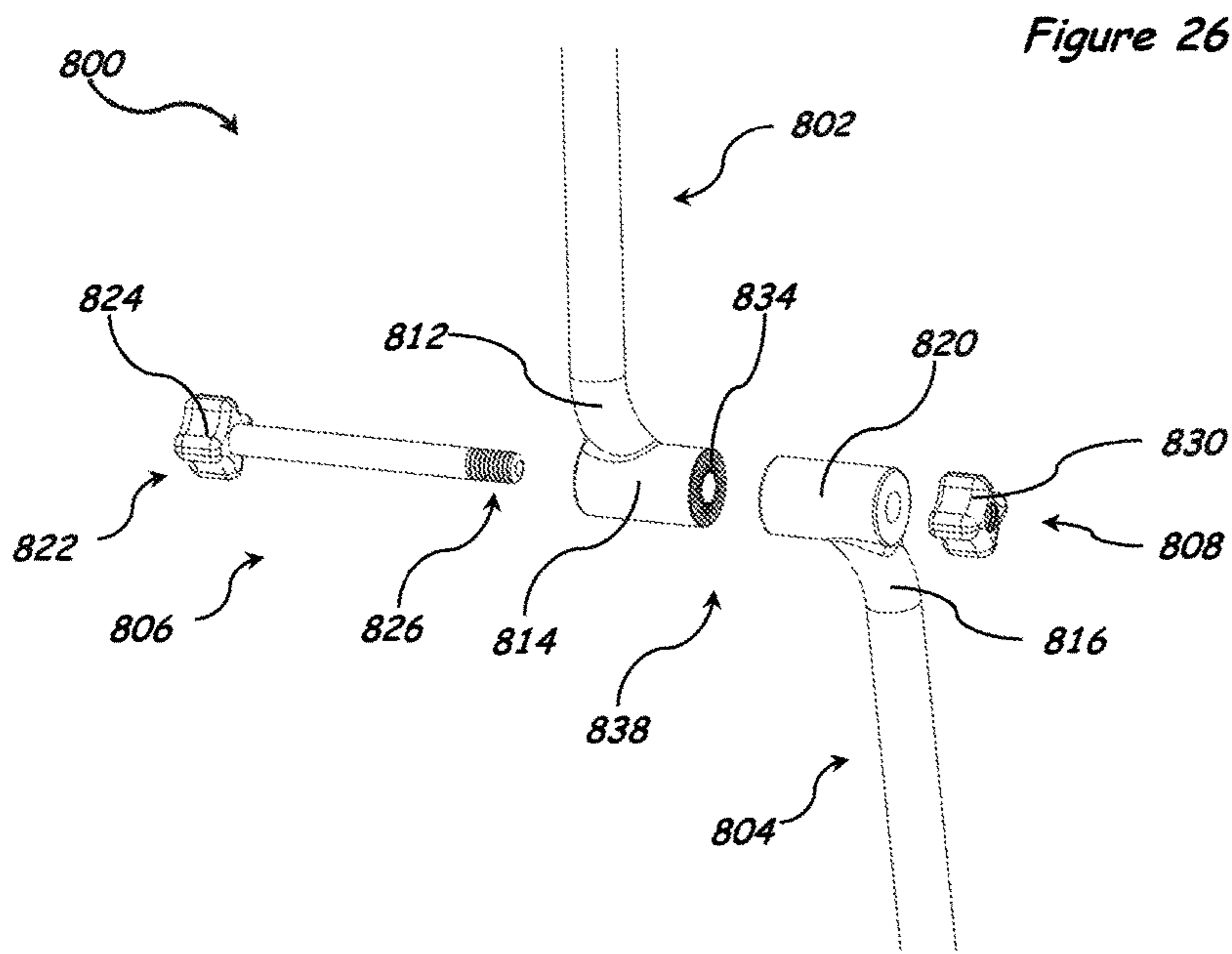


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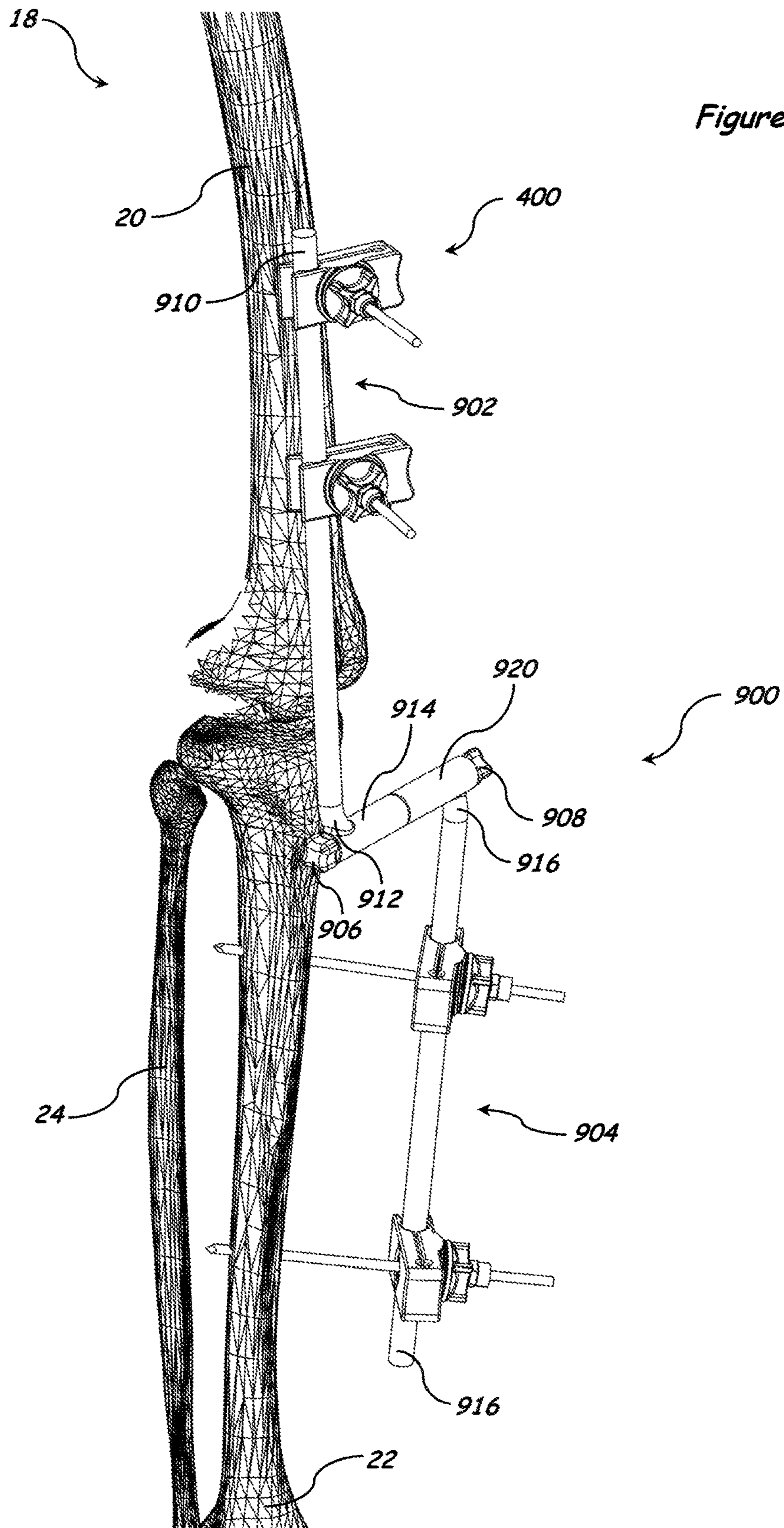
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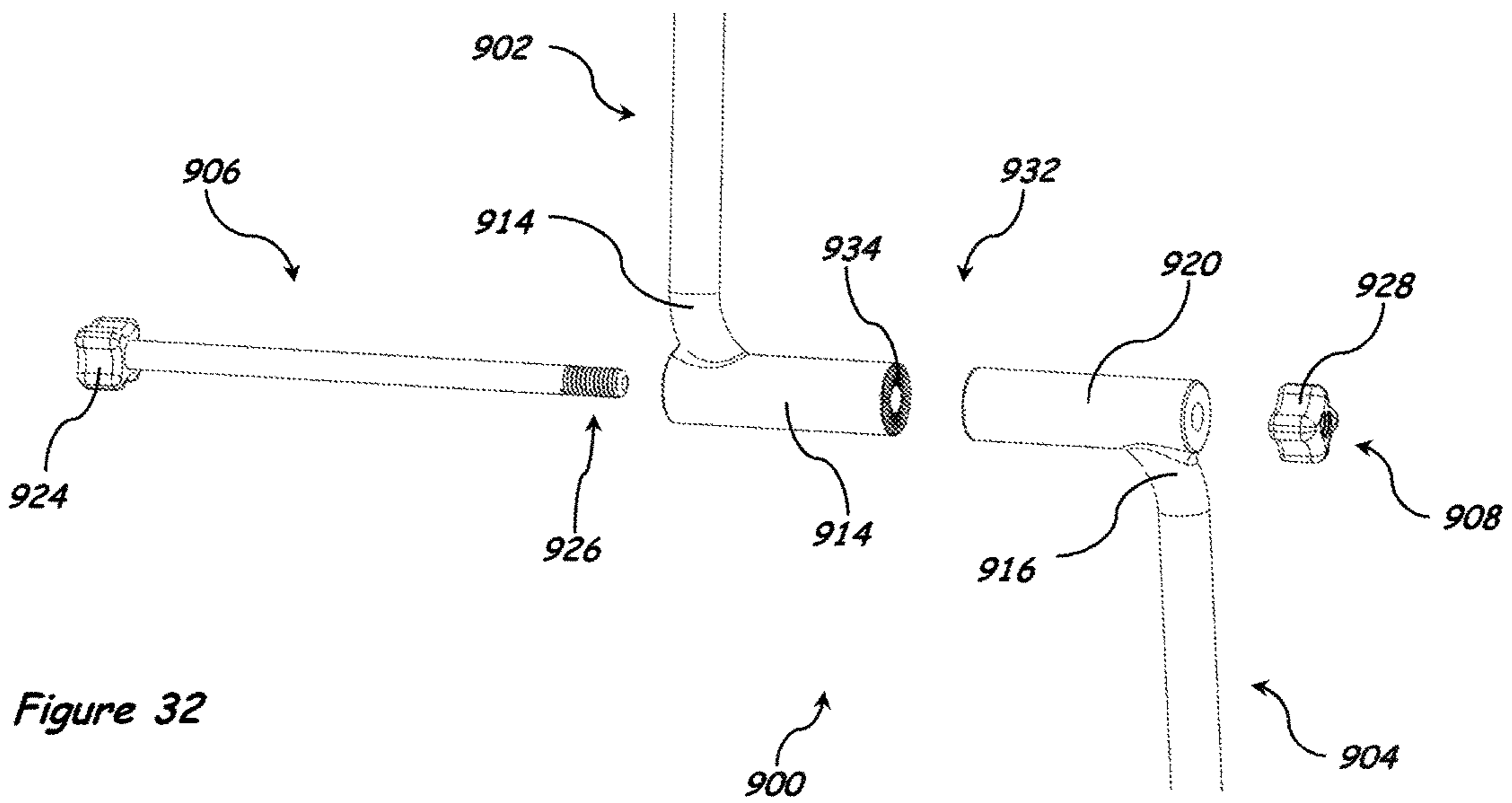
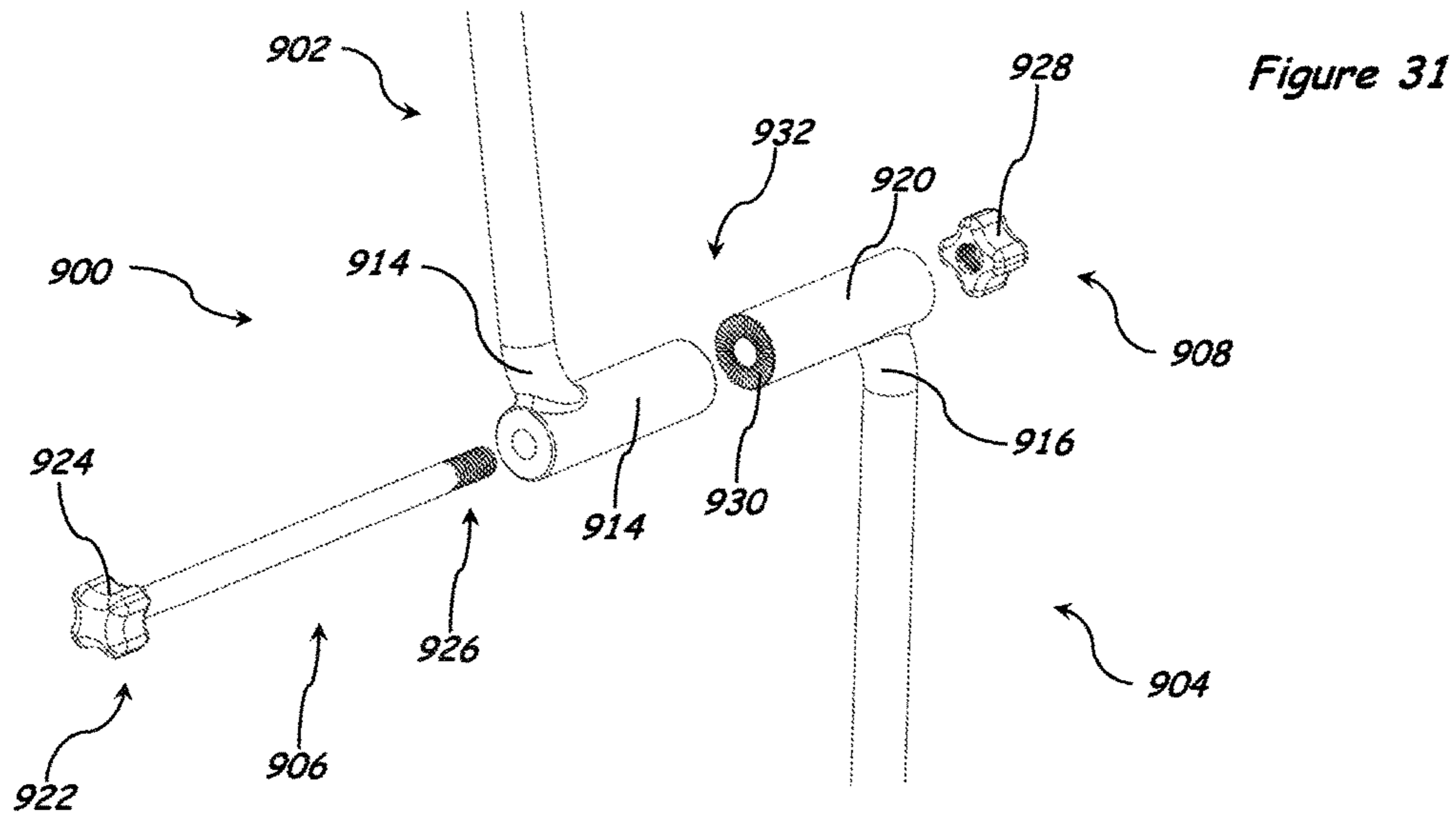






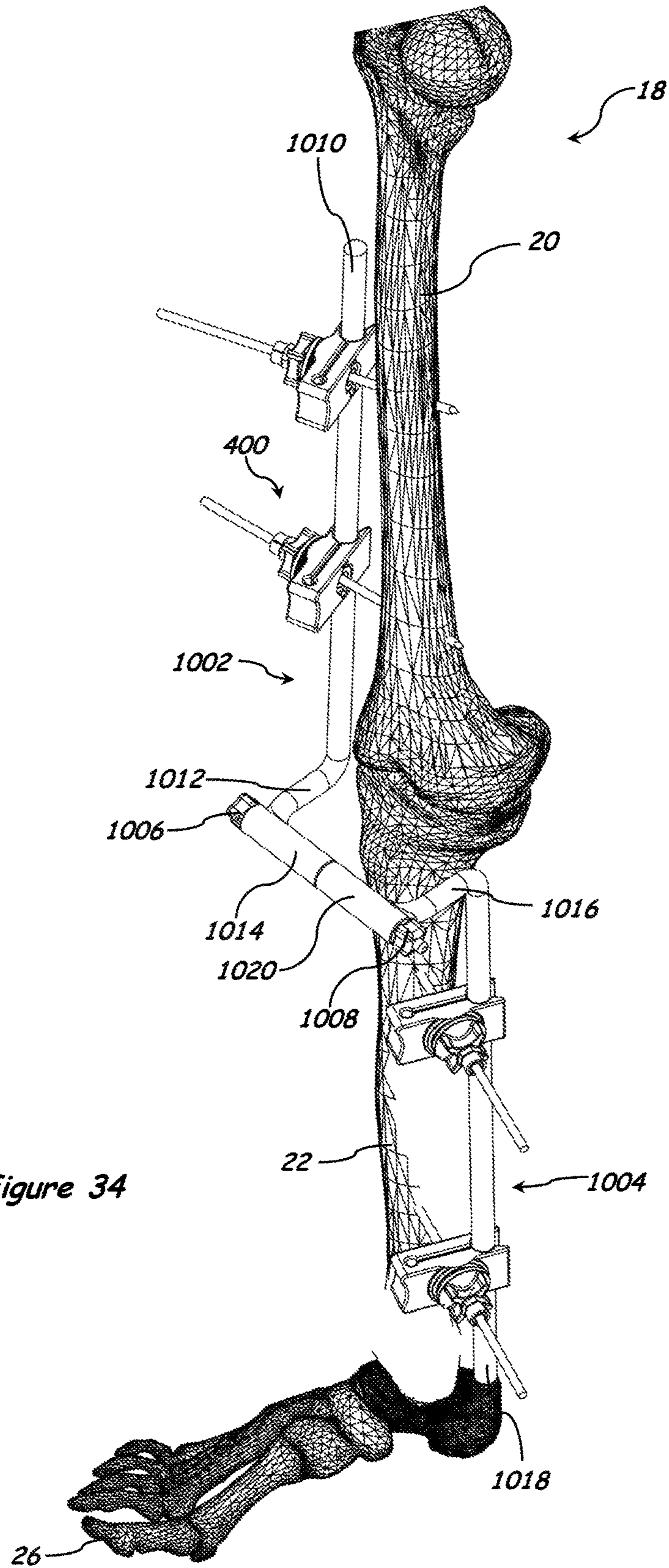


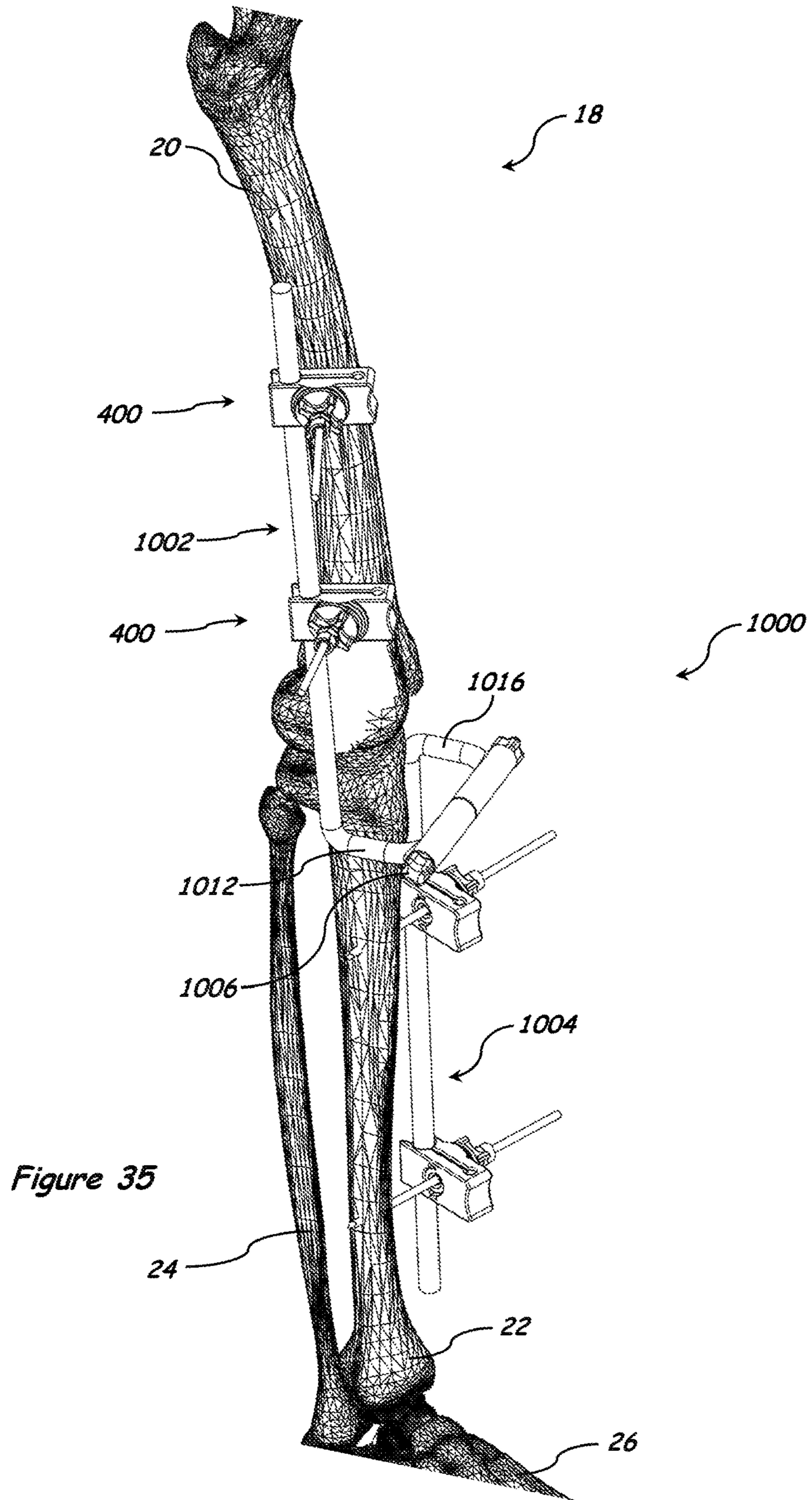












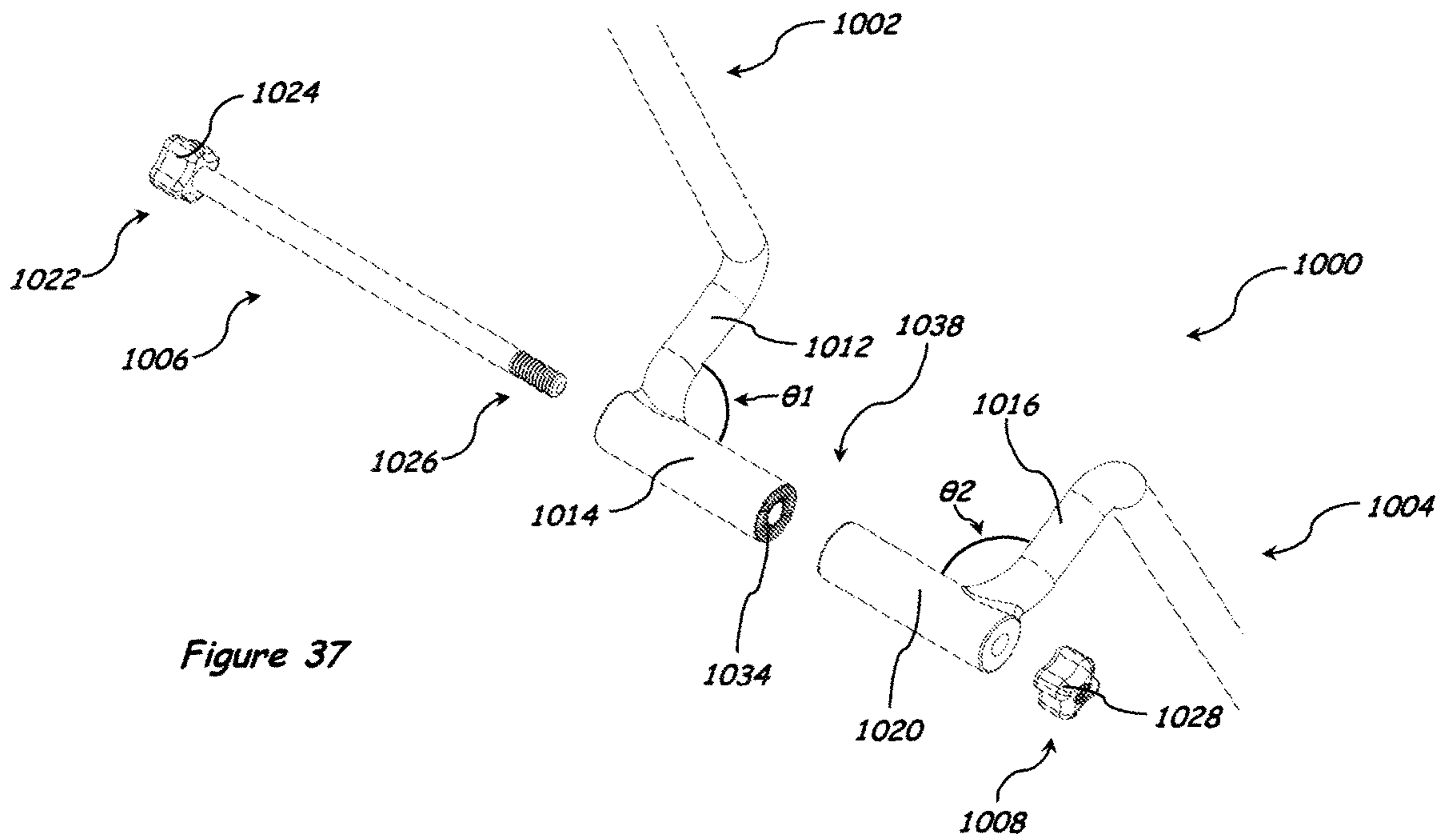
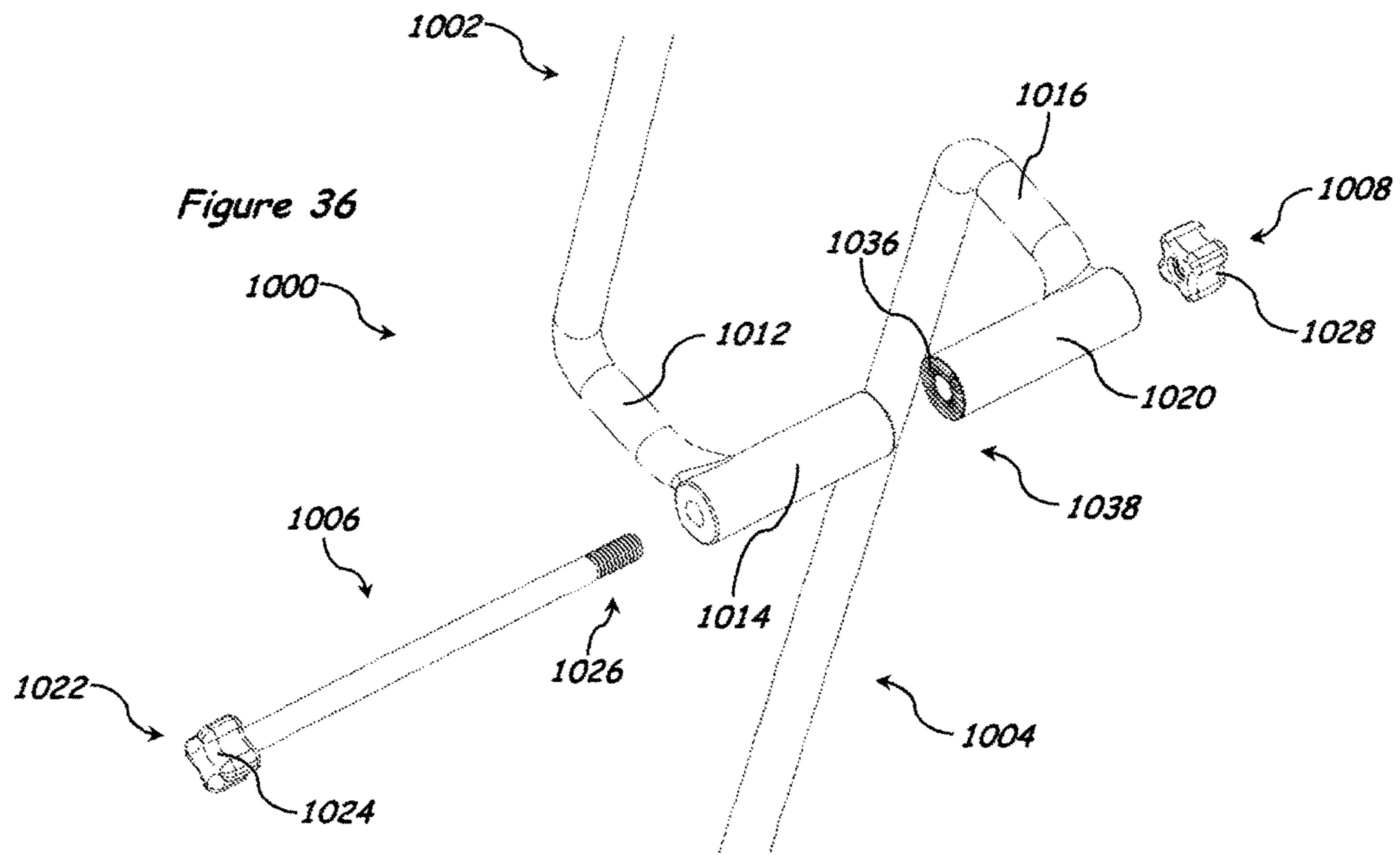
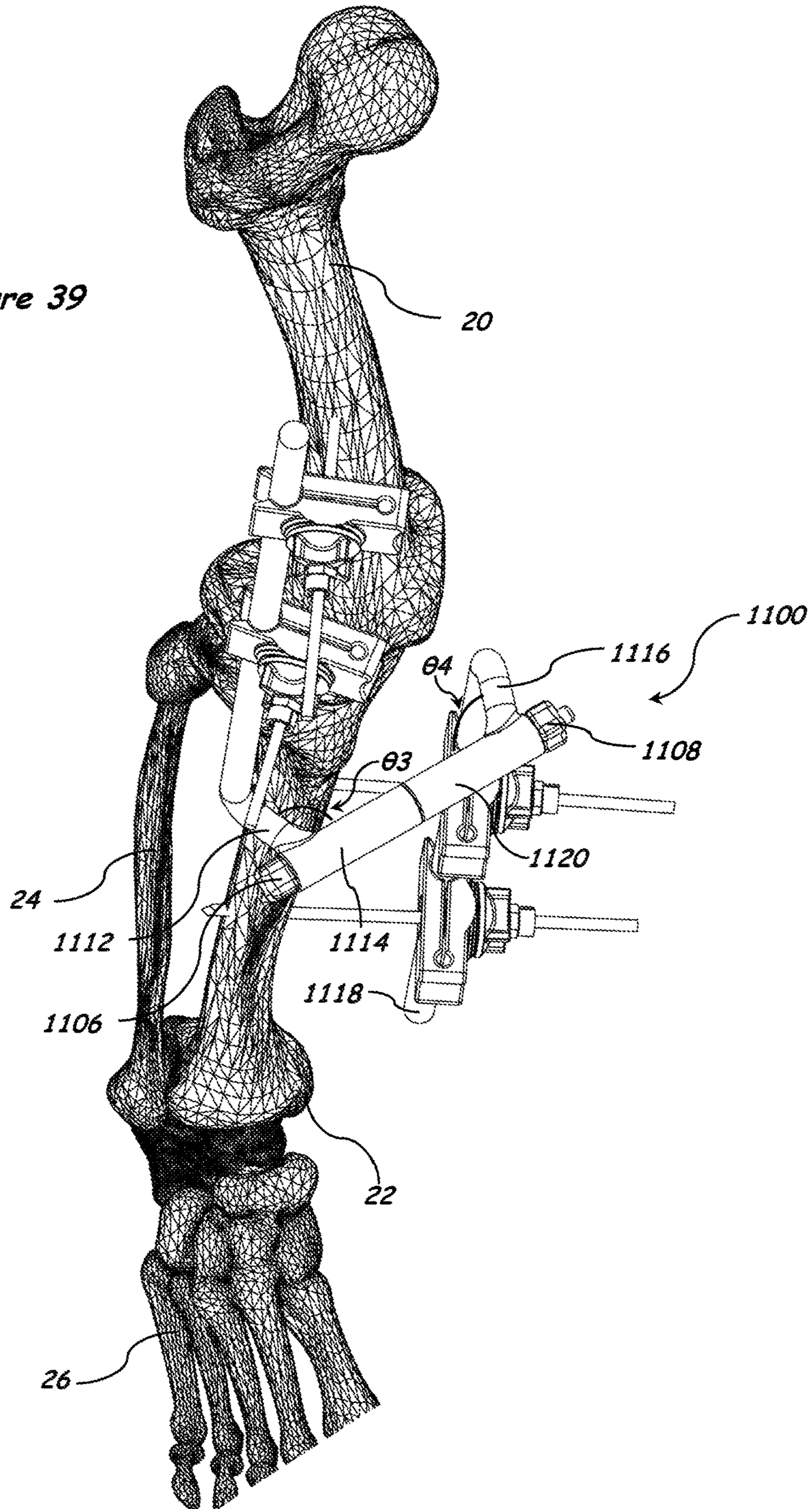




Figure 39



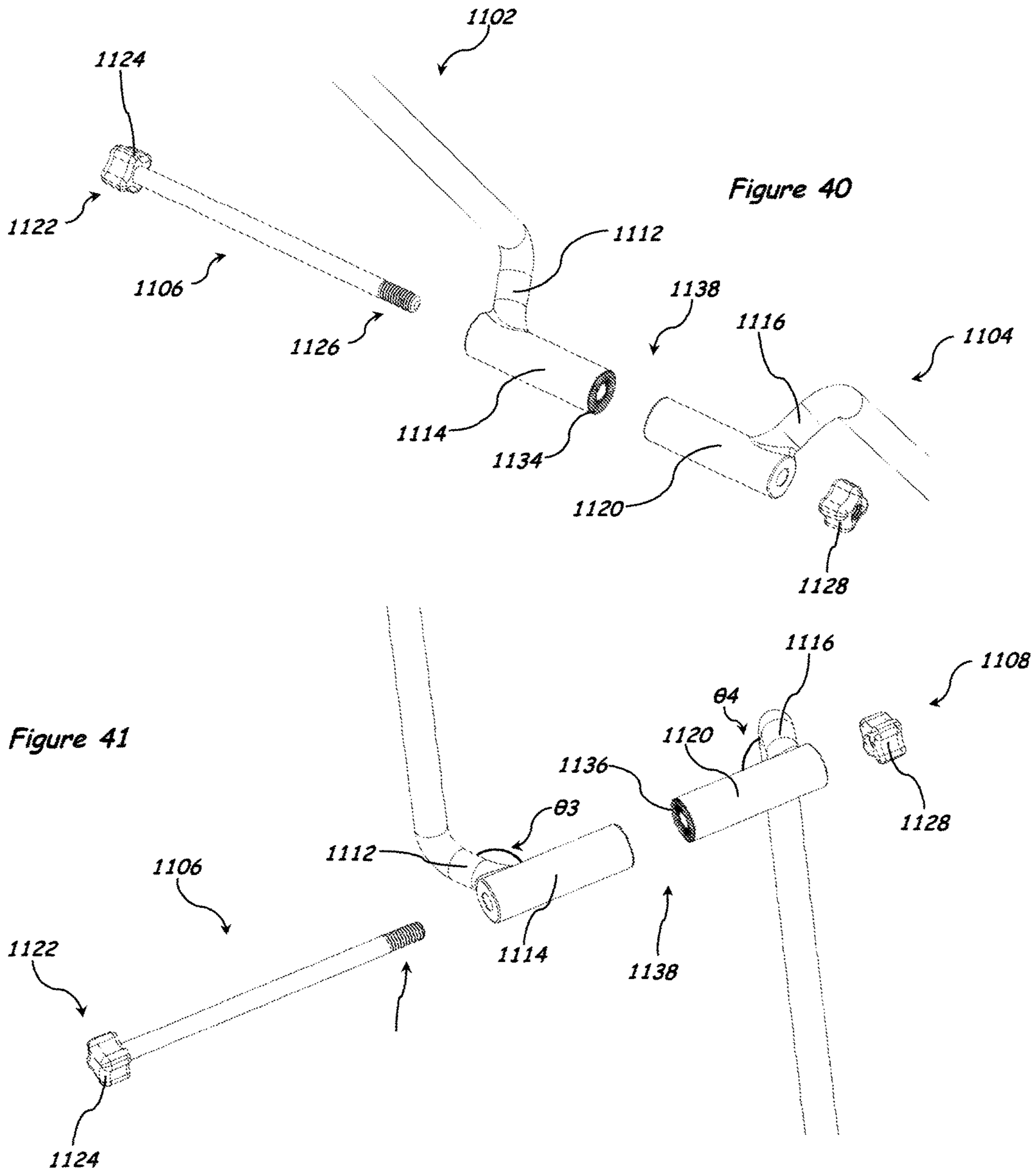
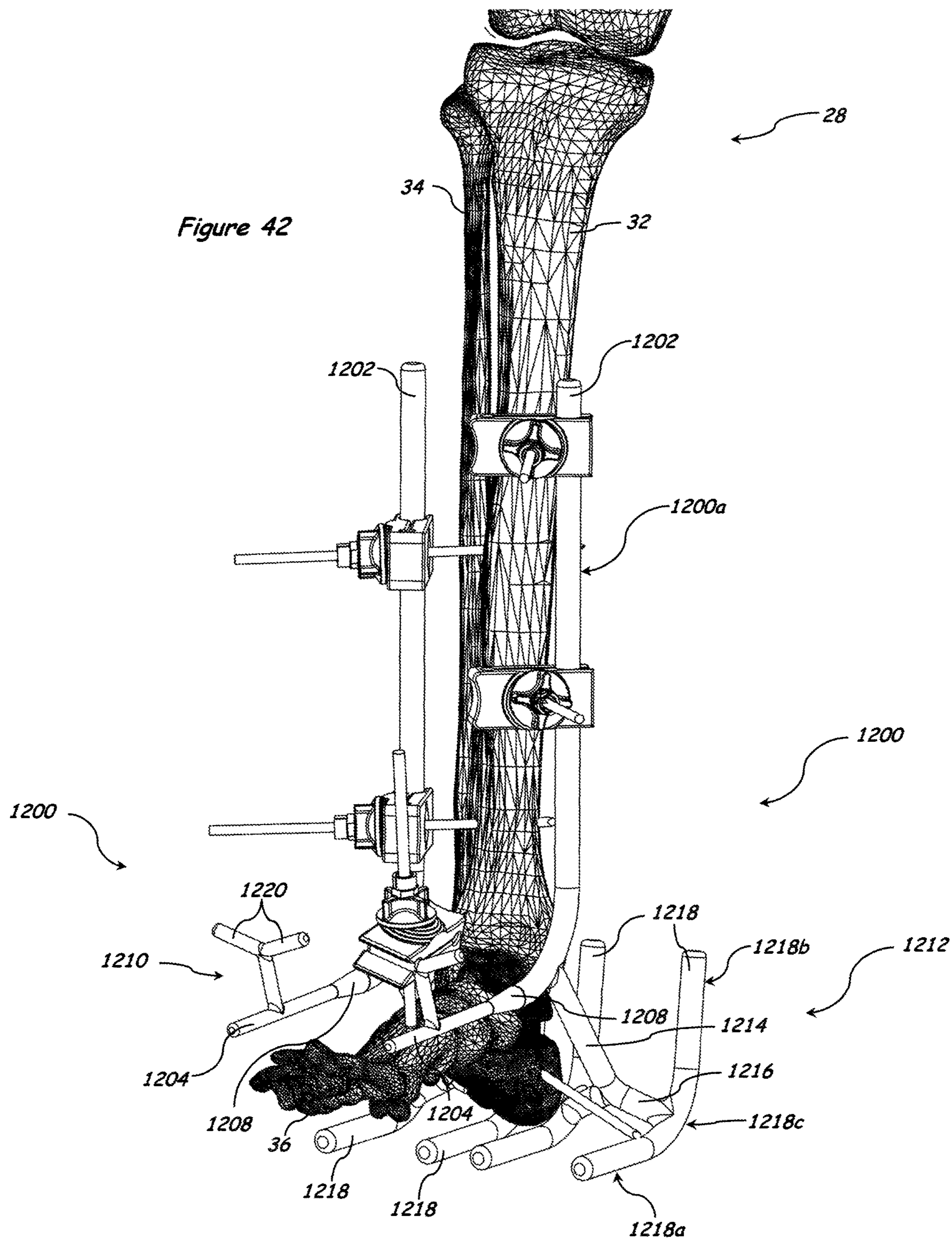
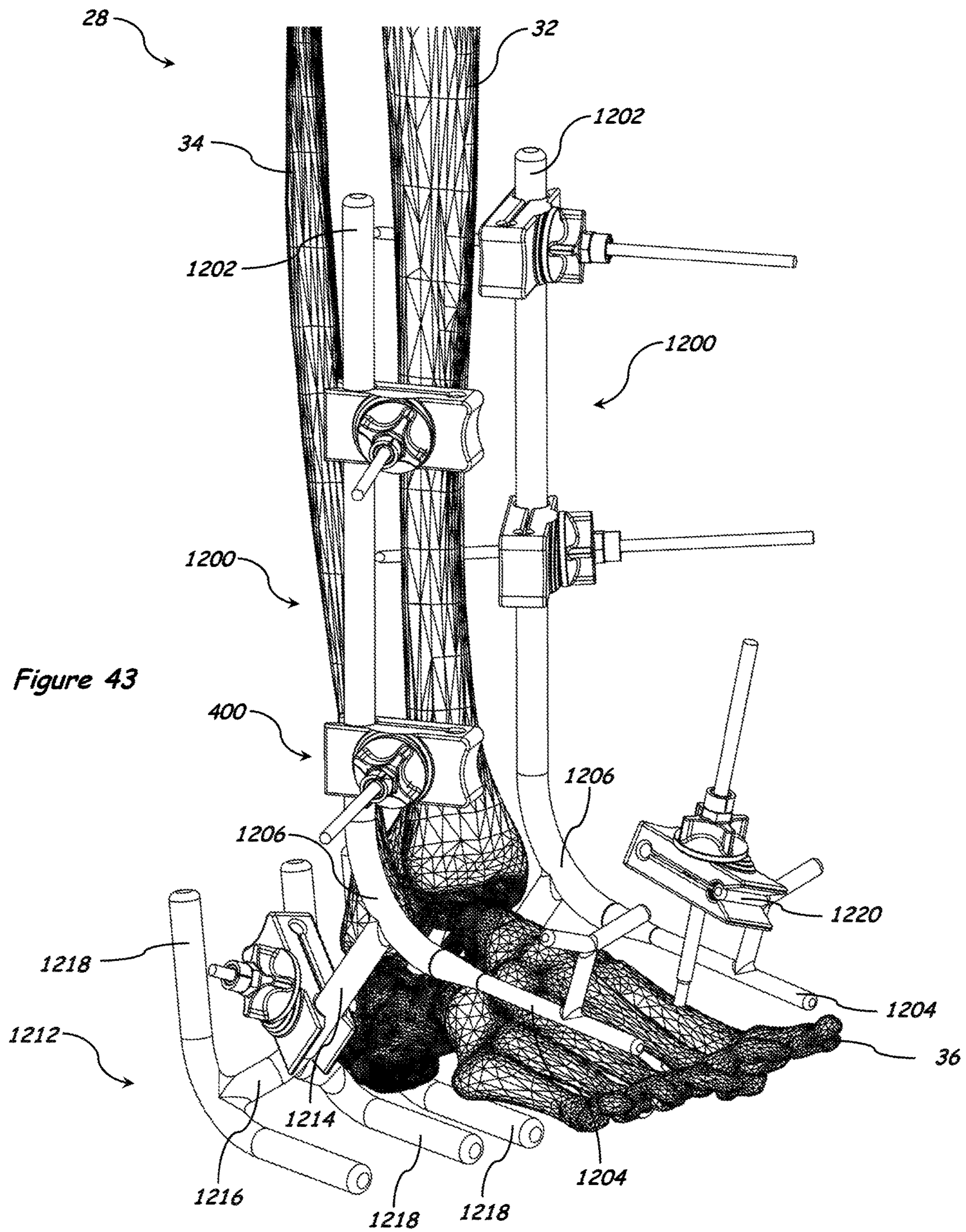


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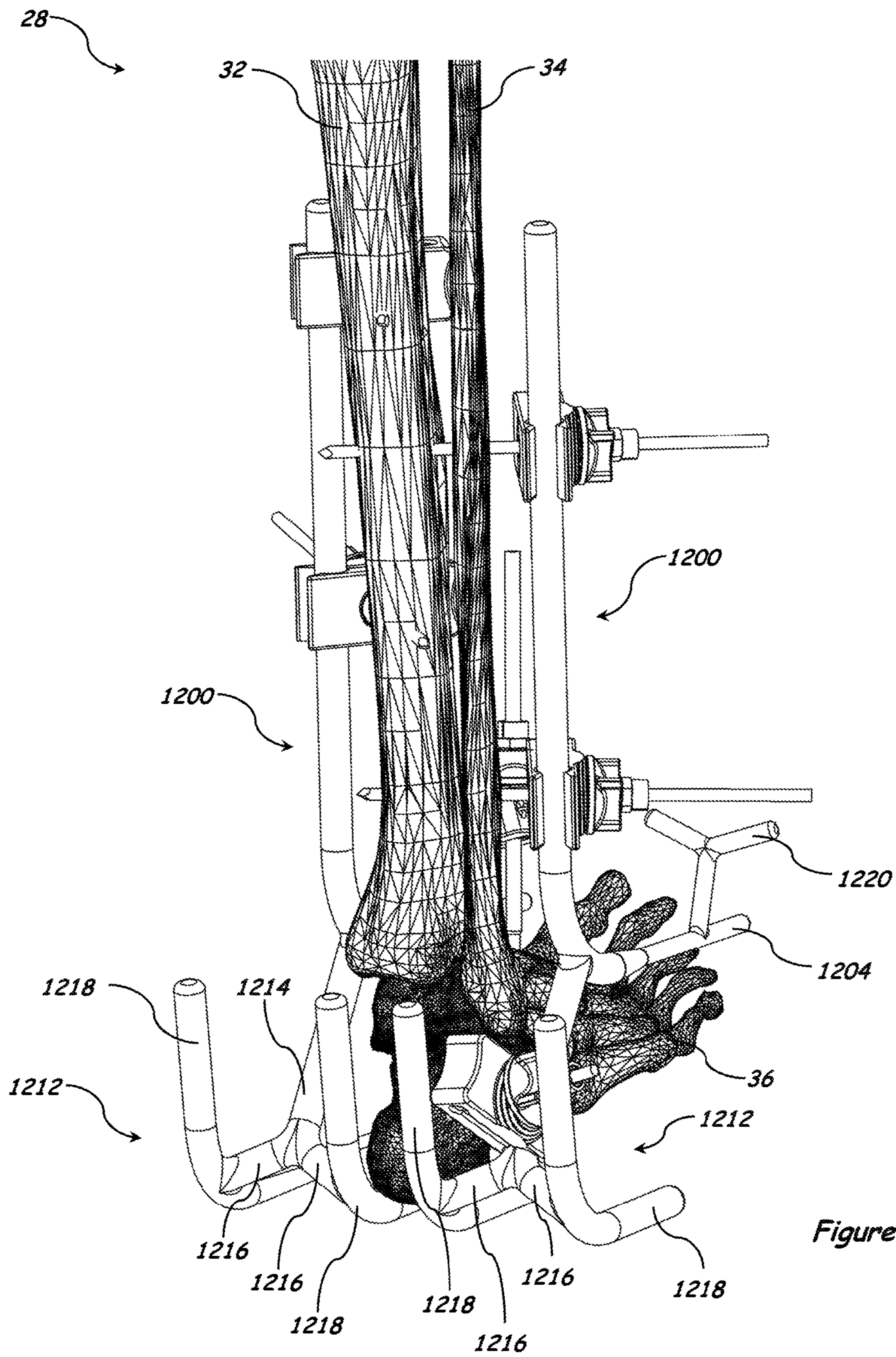
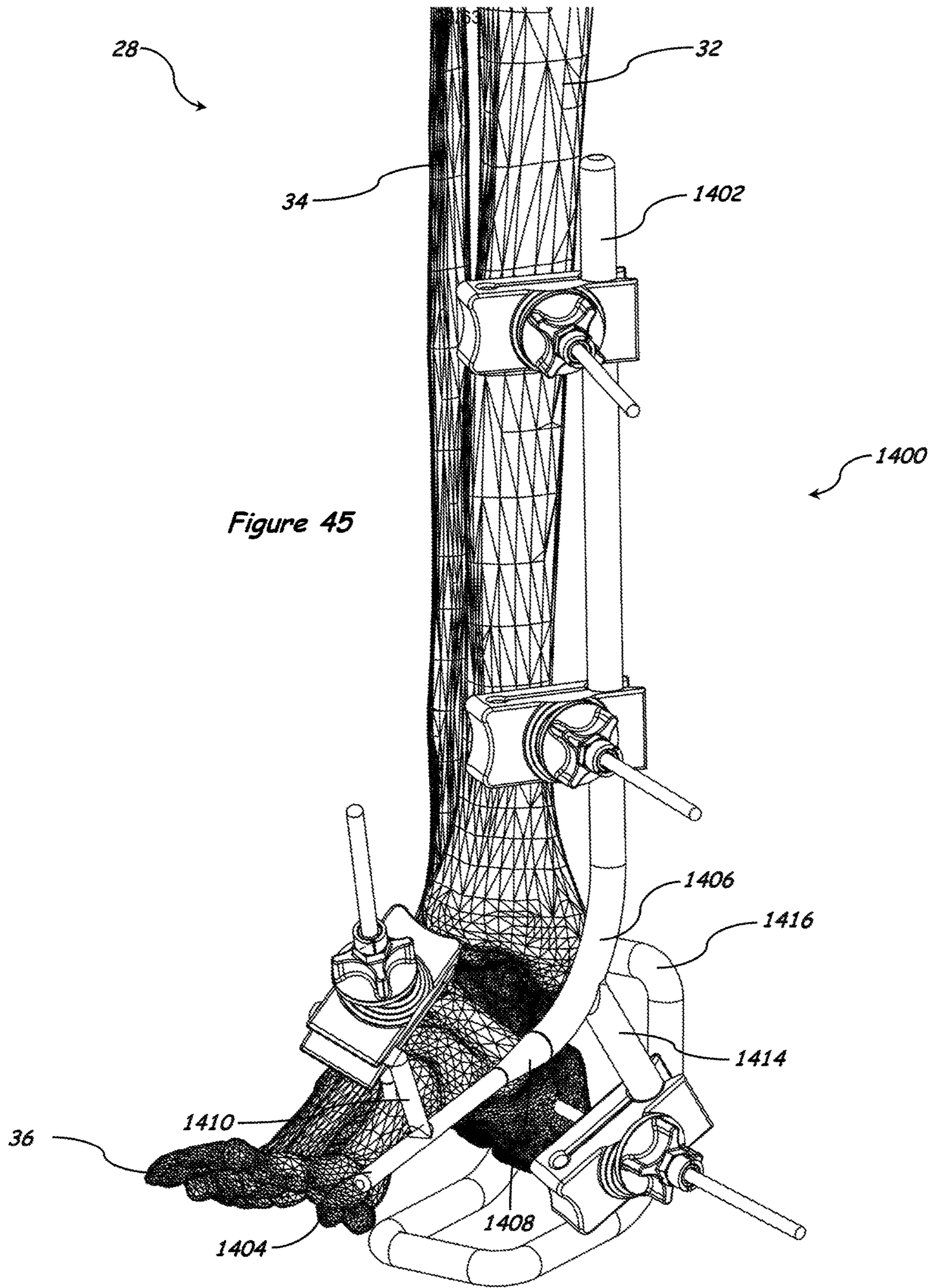
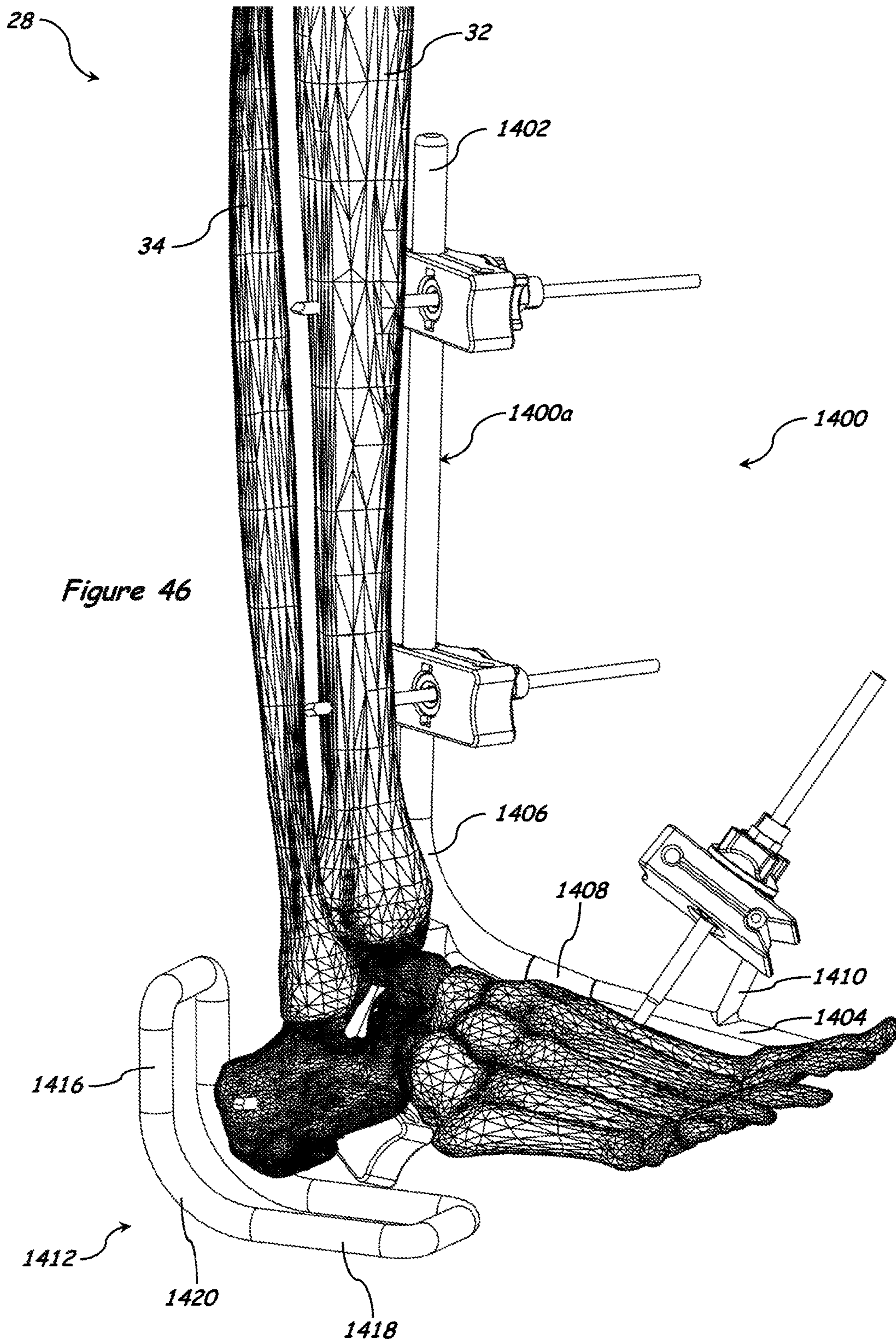


Figure 44





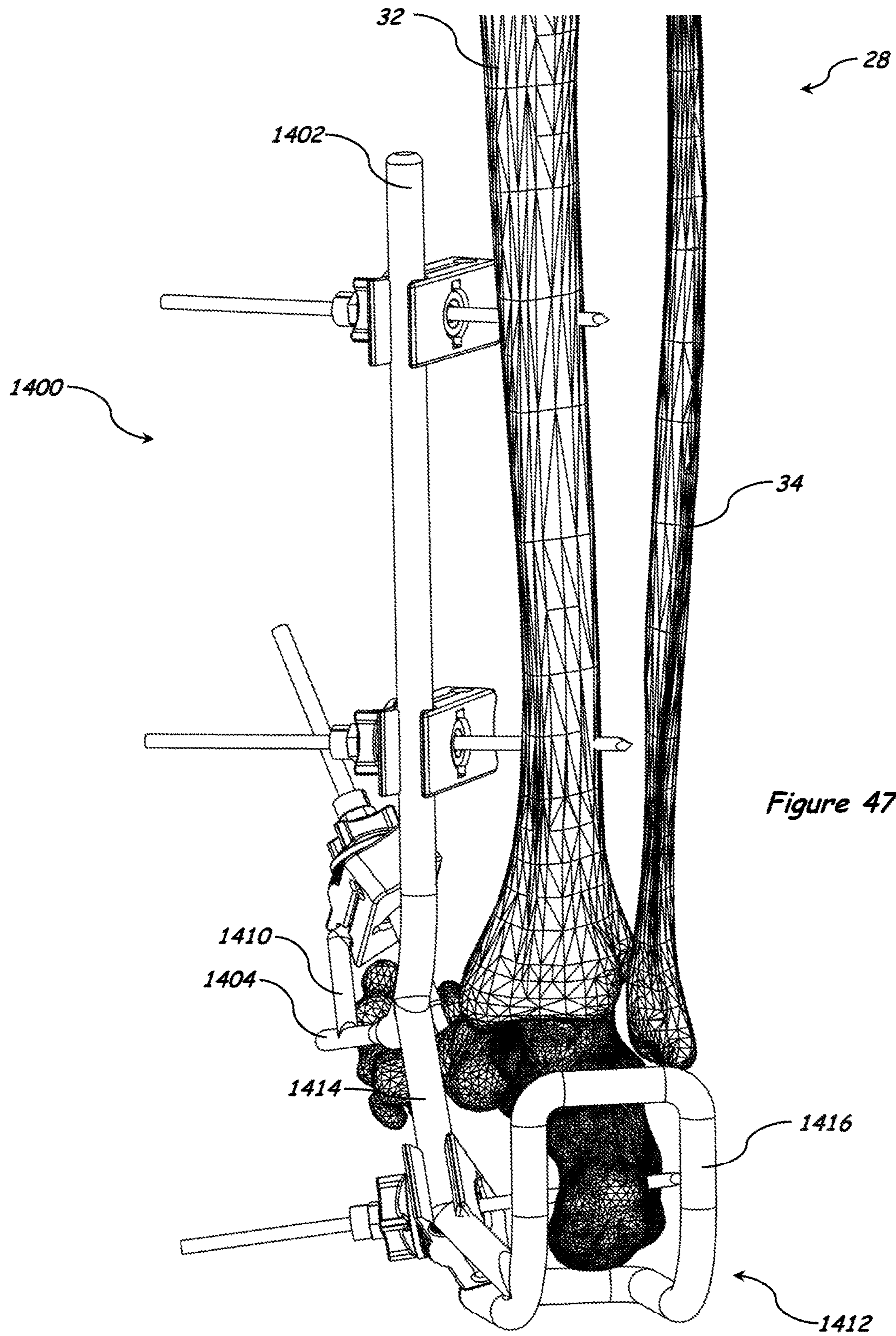
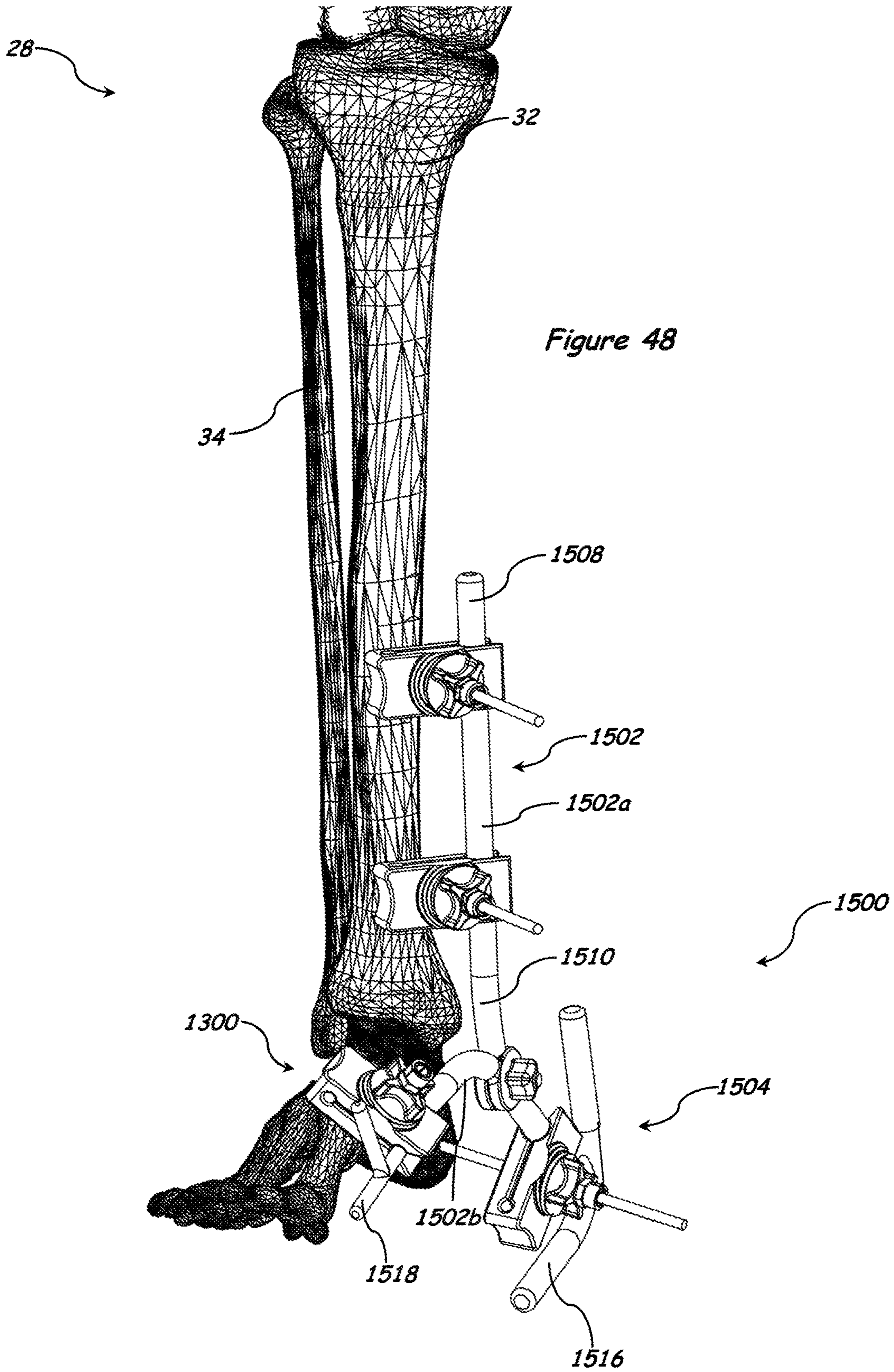
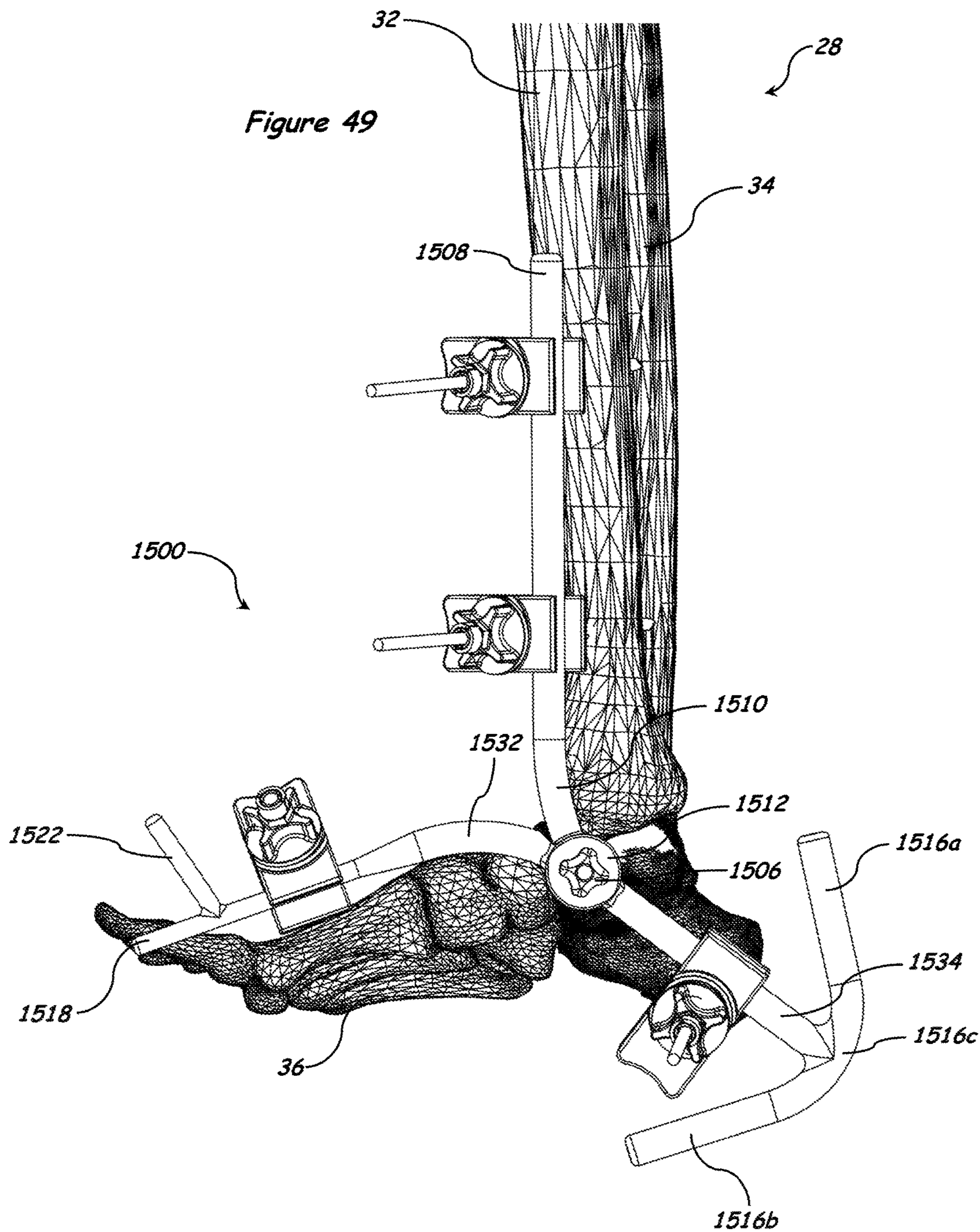


Figure 47









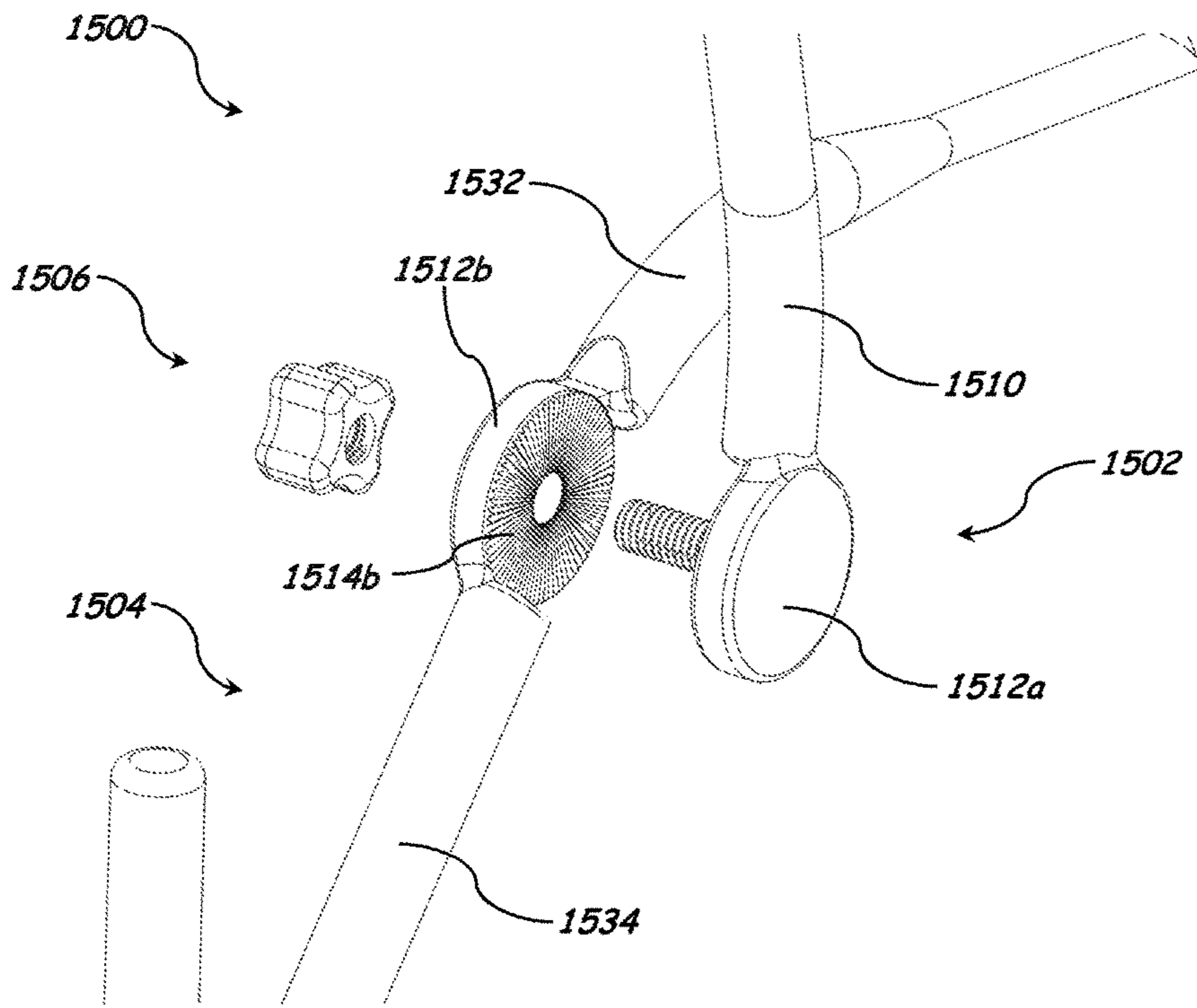


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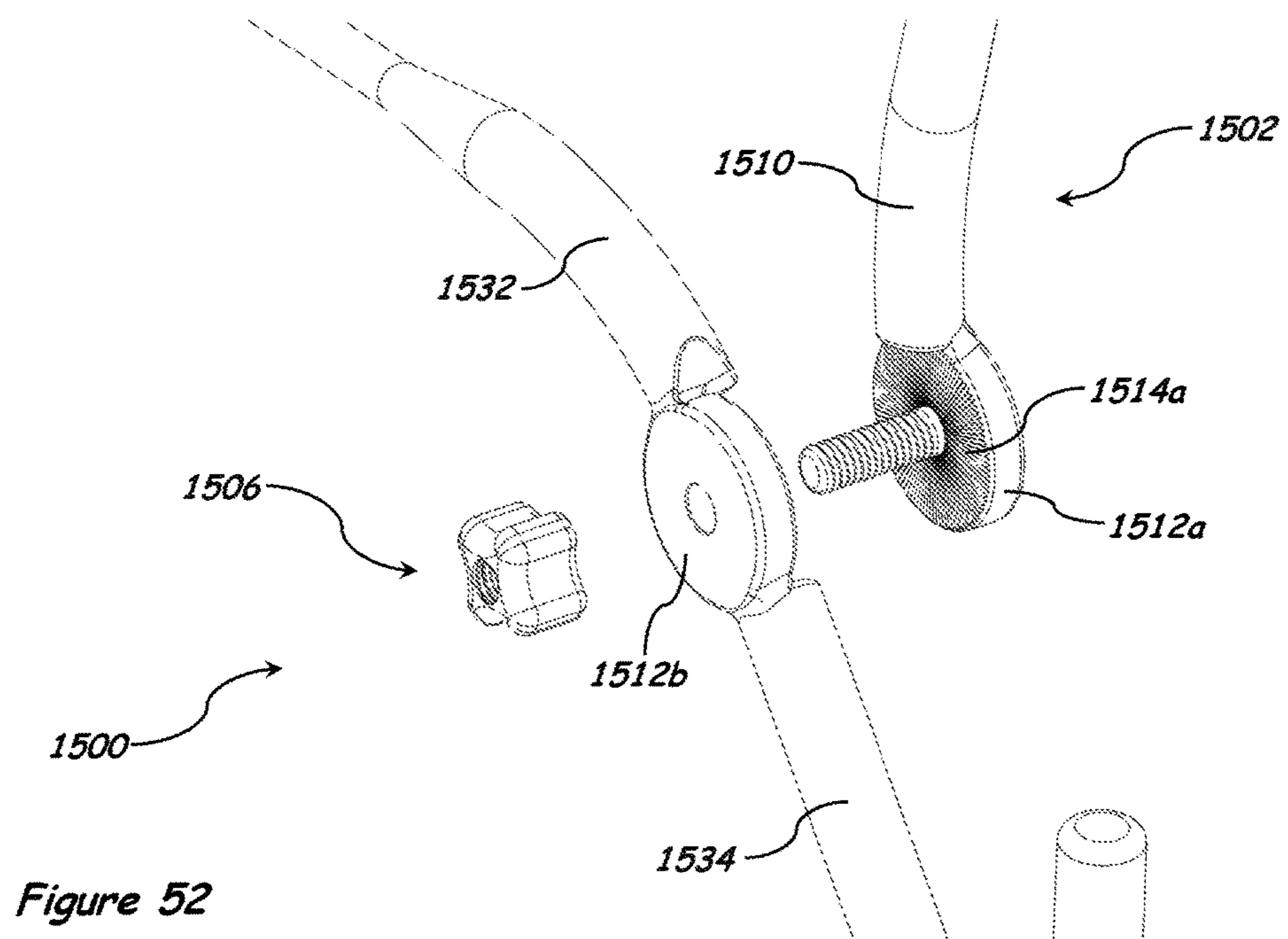
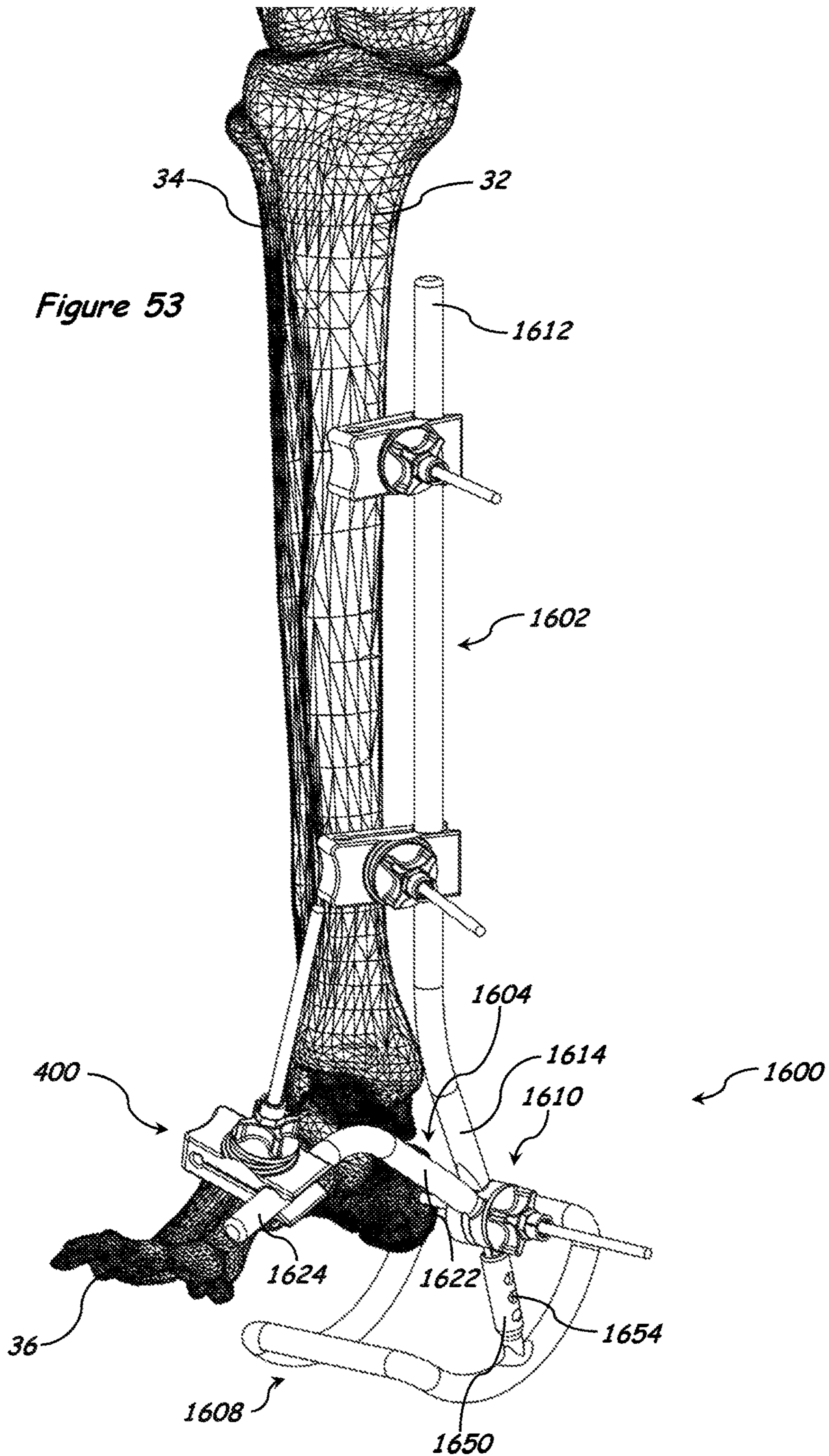


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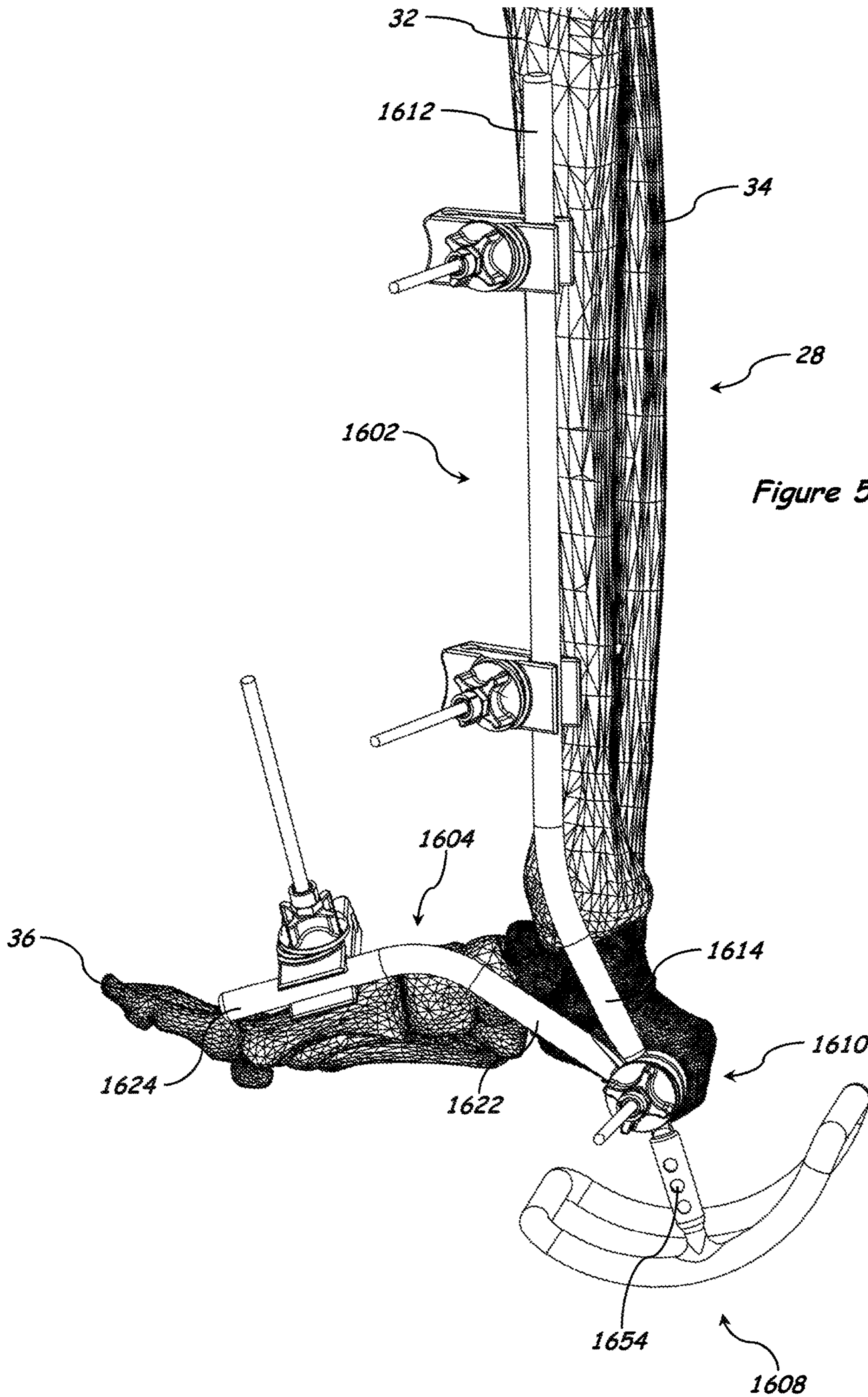


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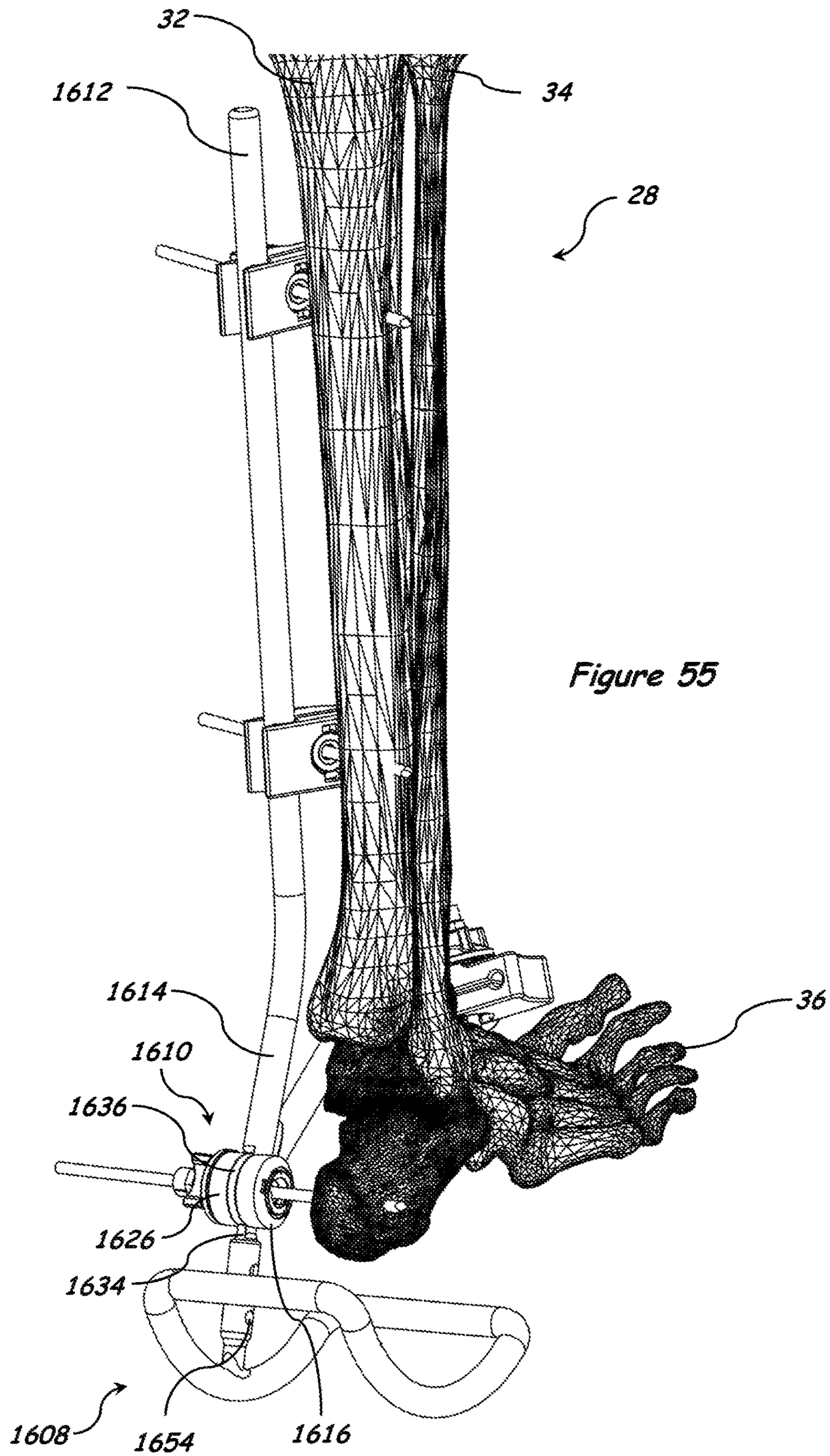
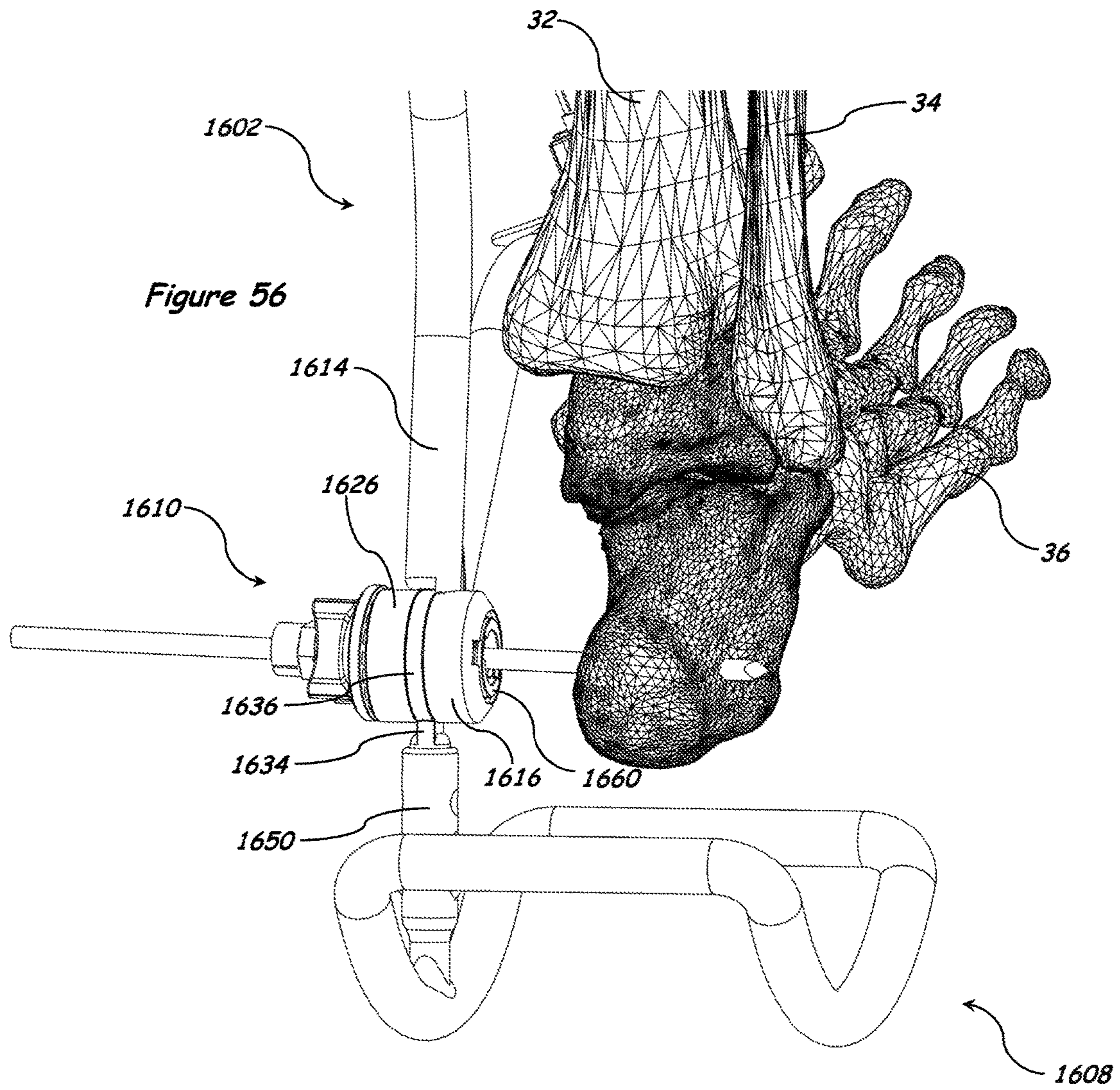
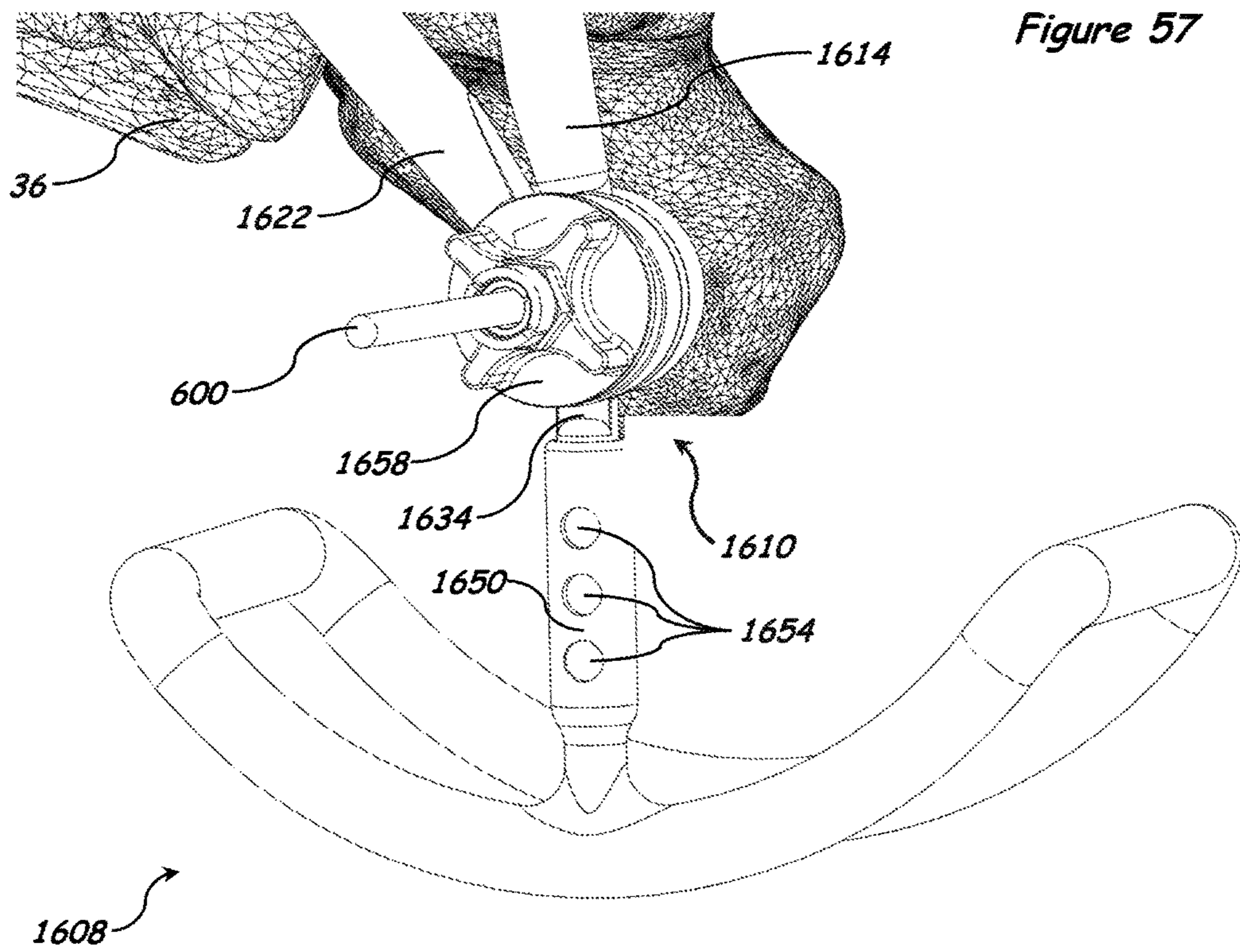
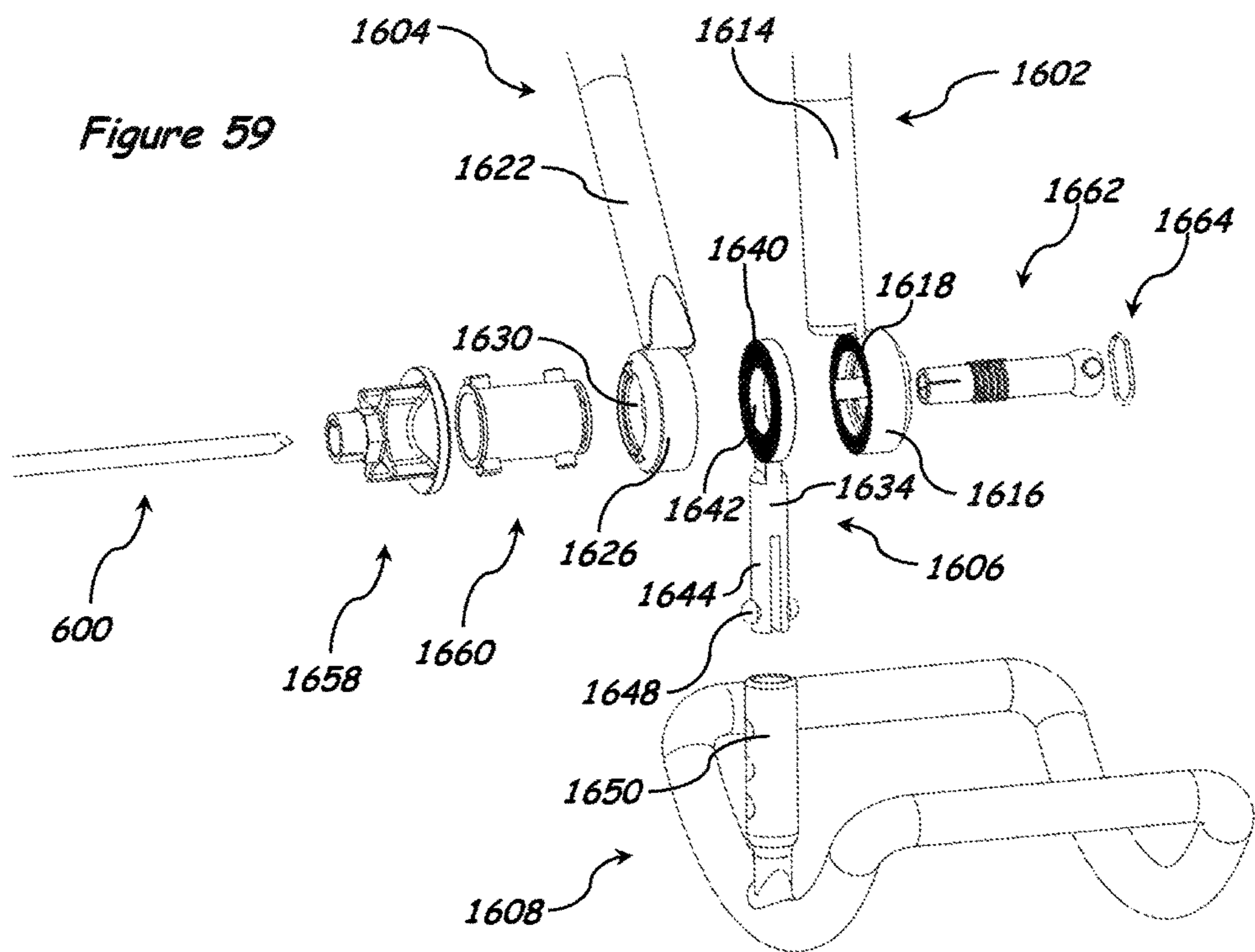
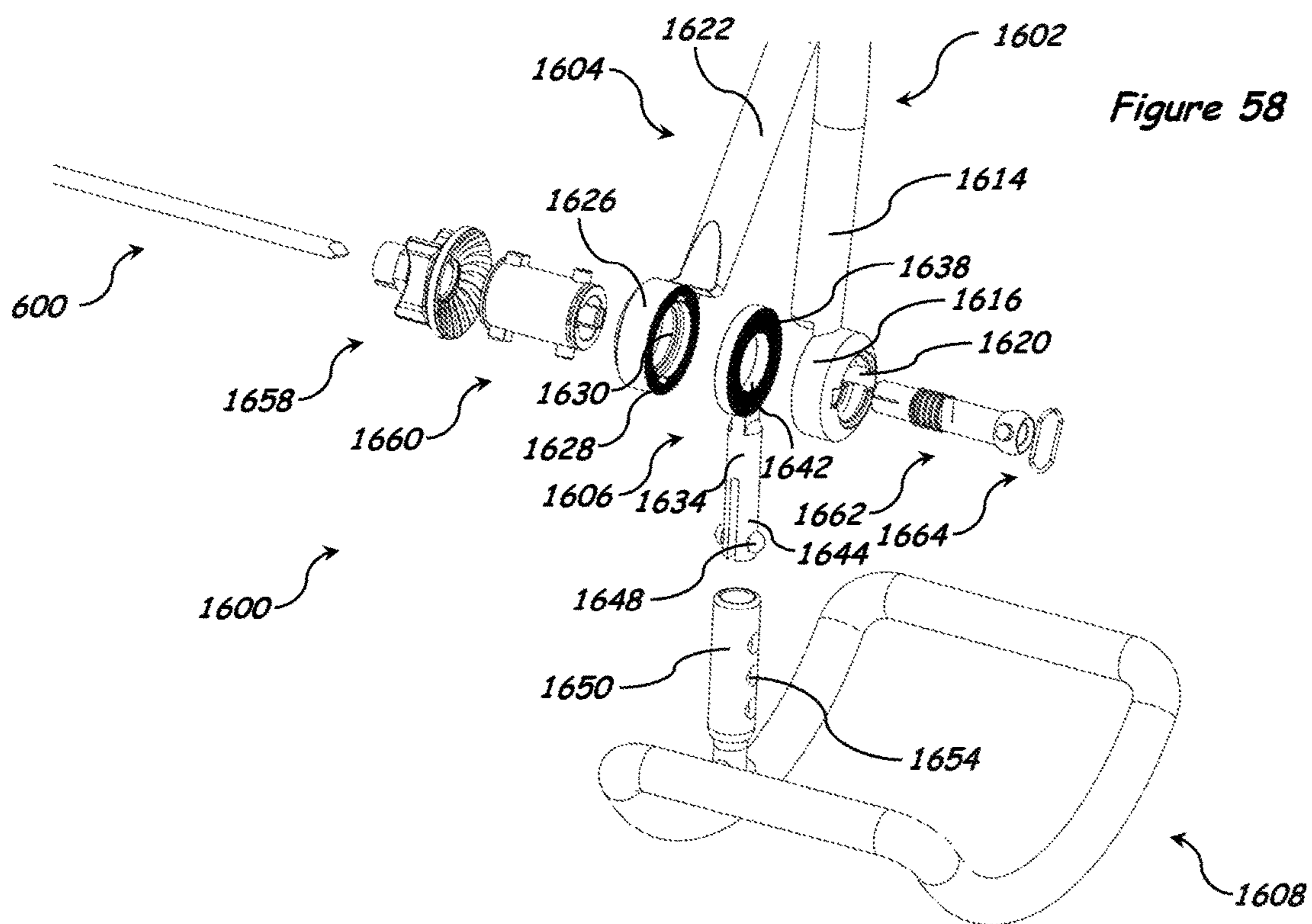
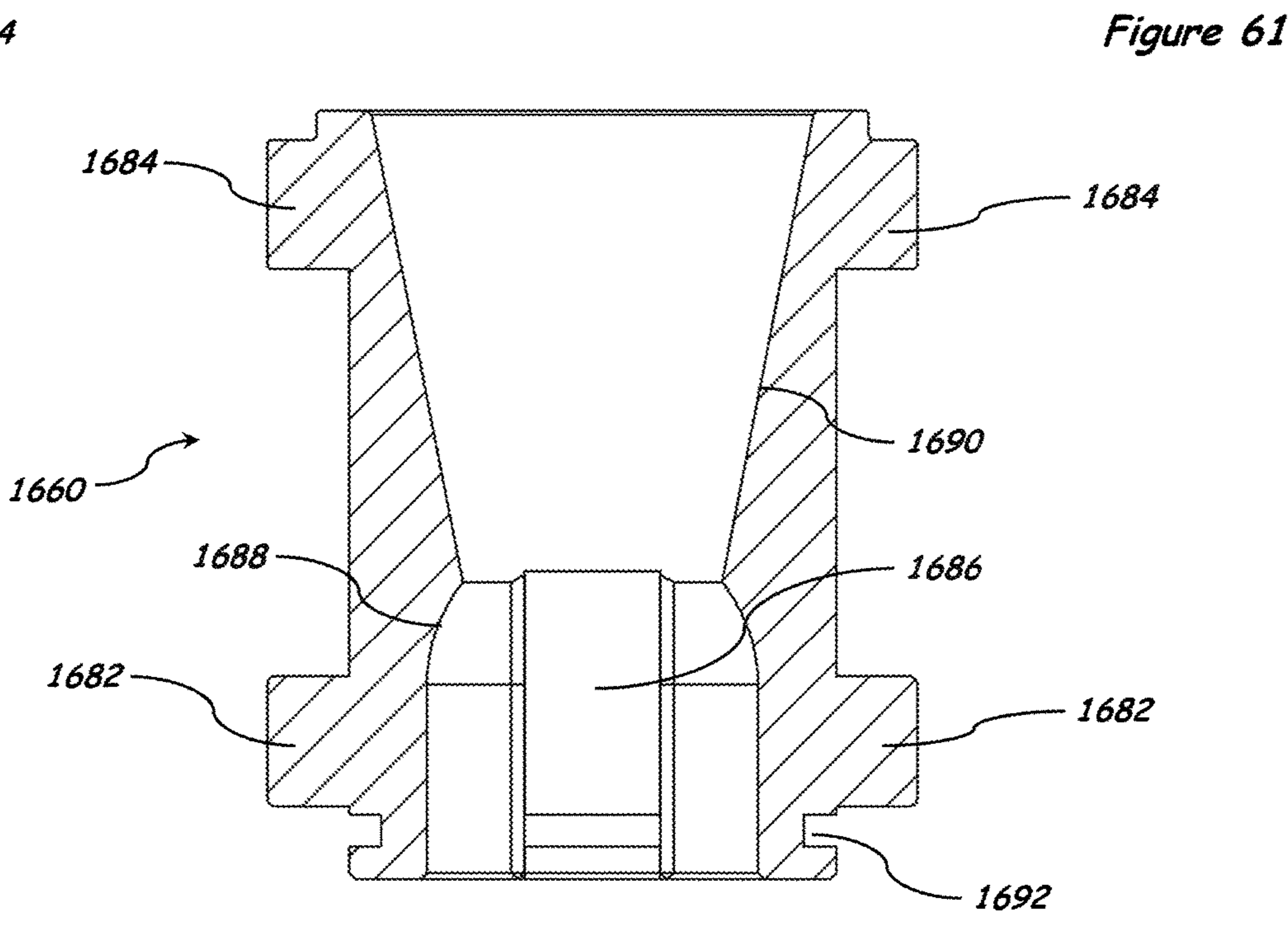
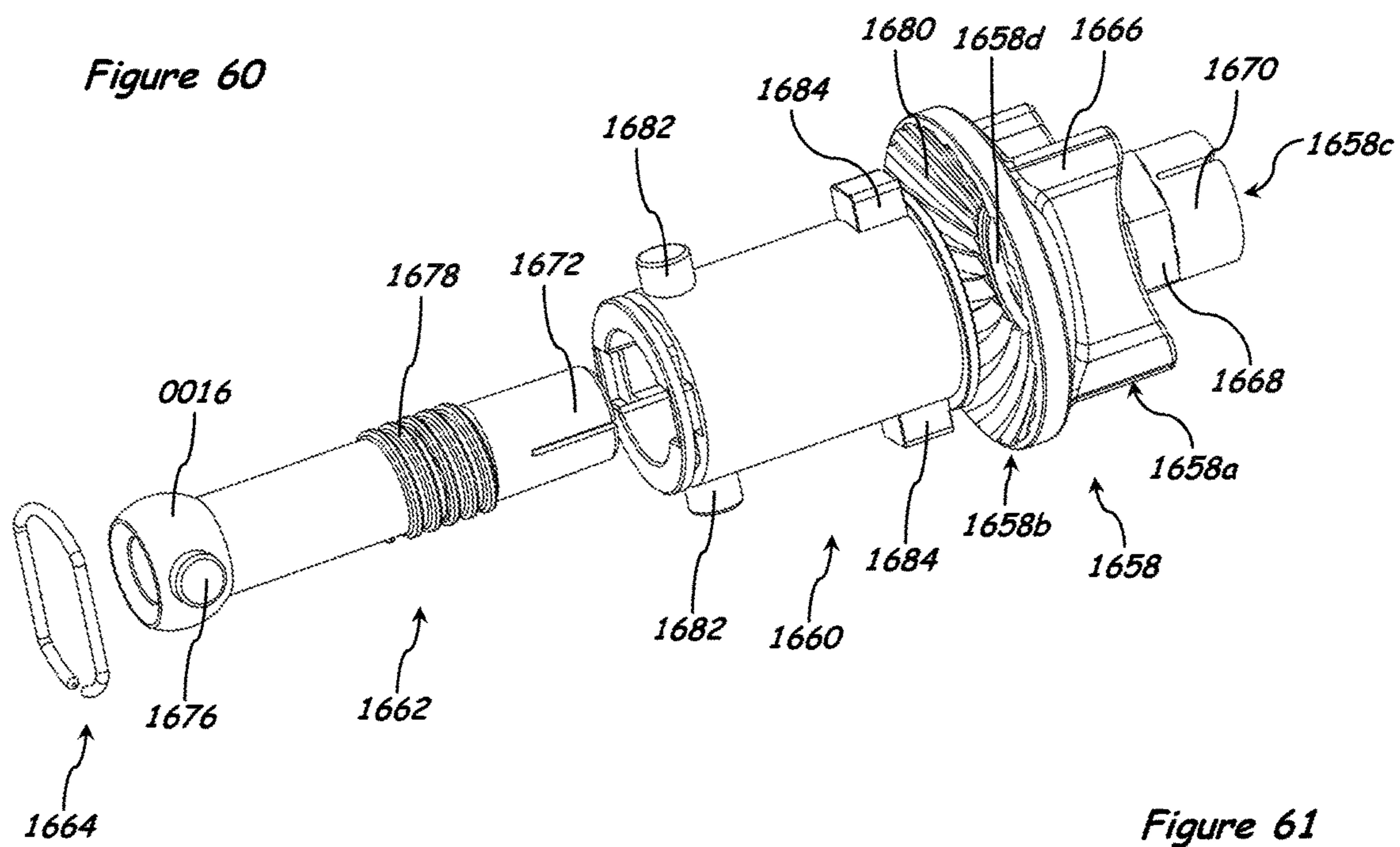


Figure 55











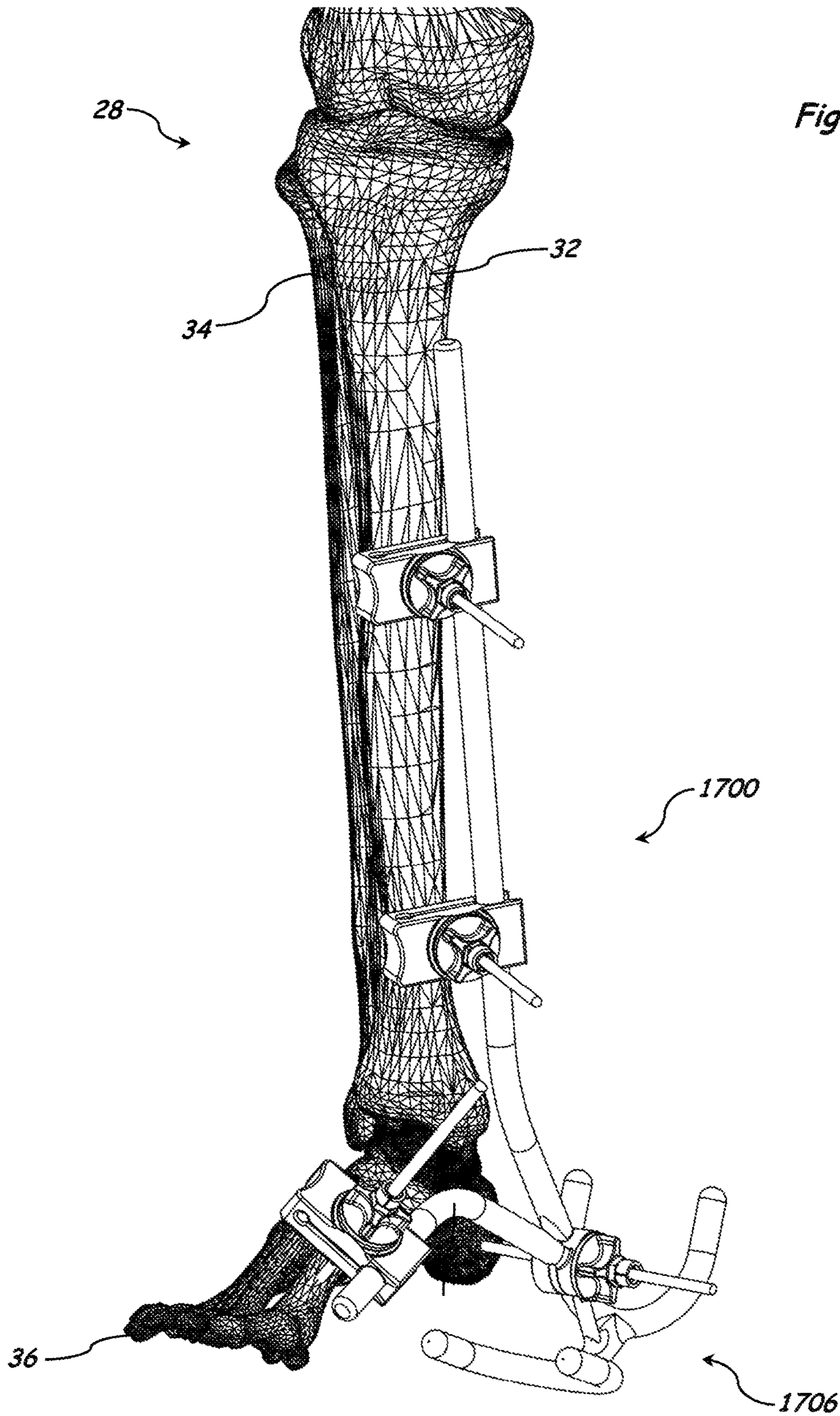
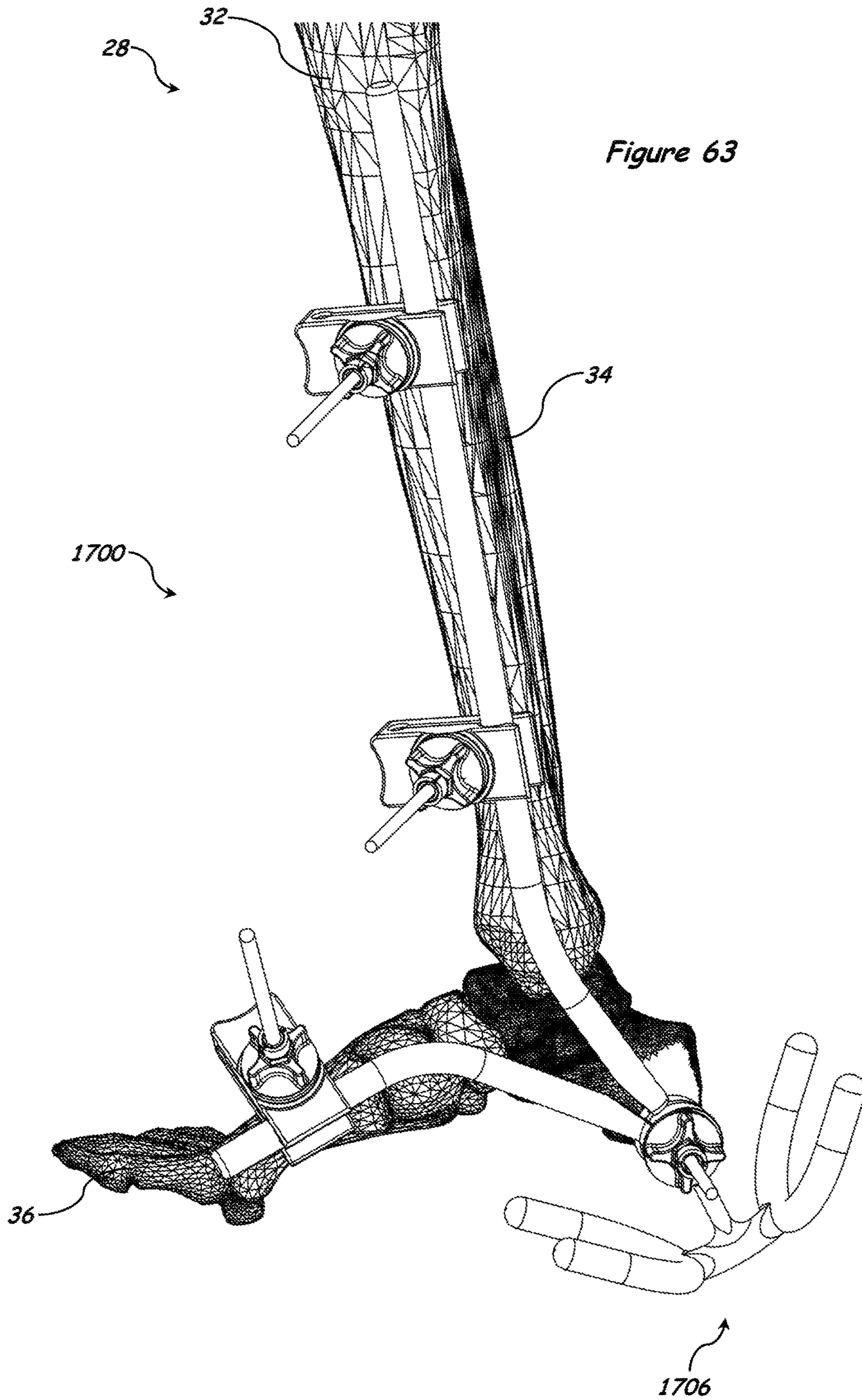
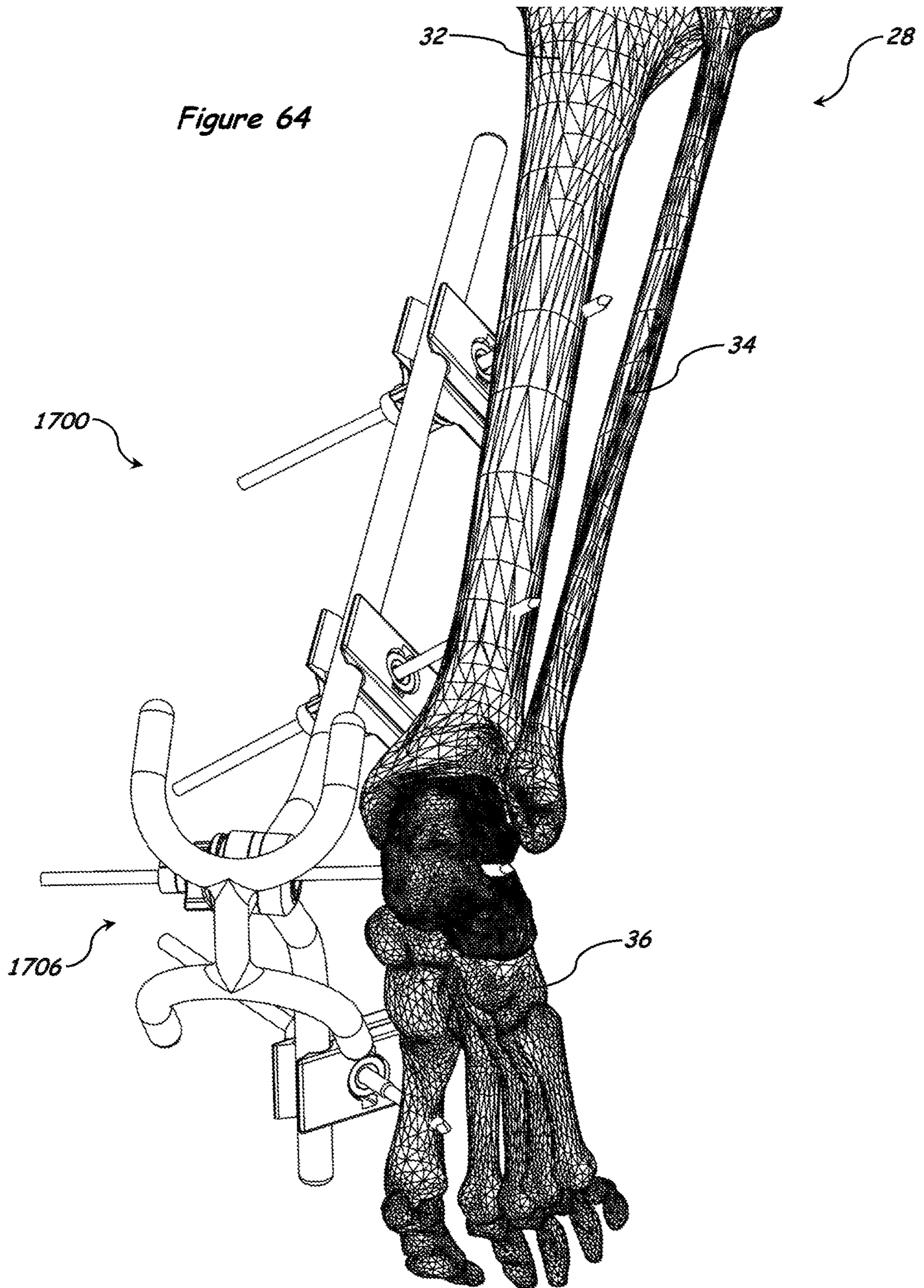
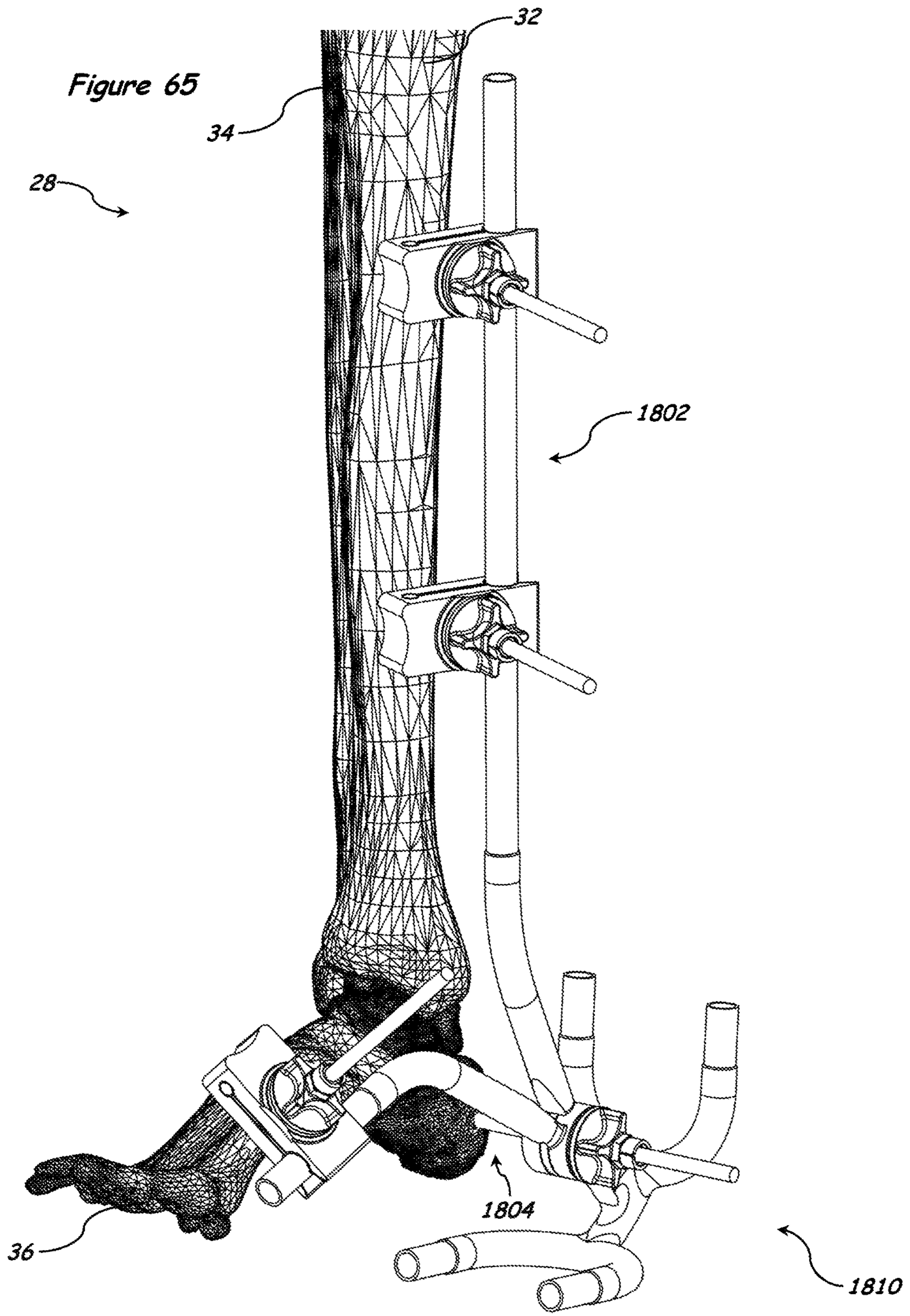


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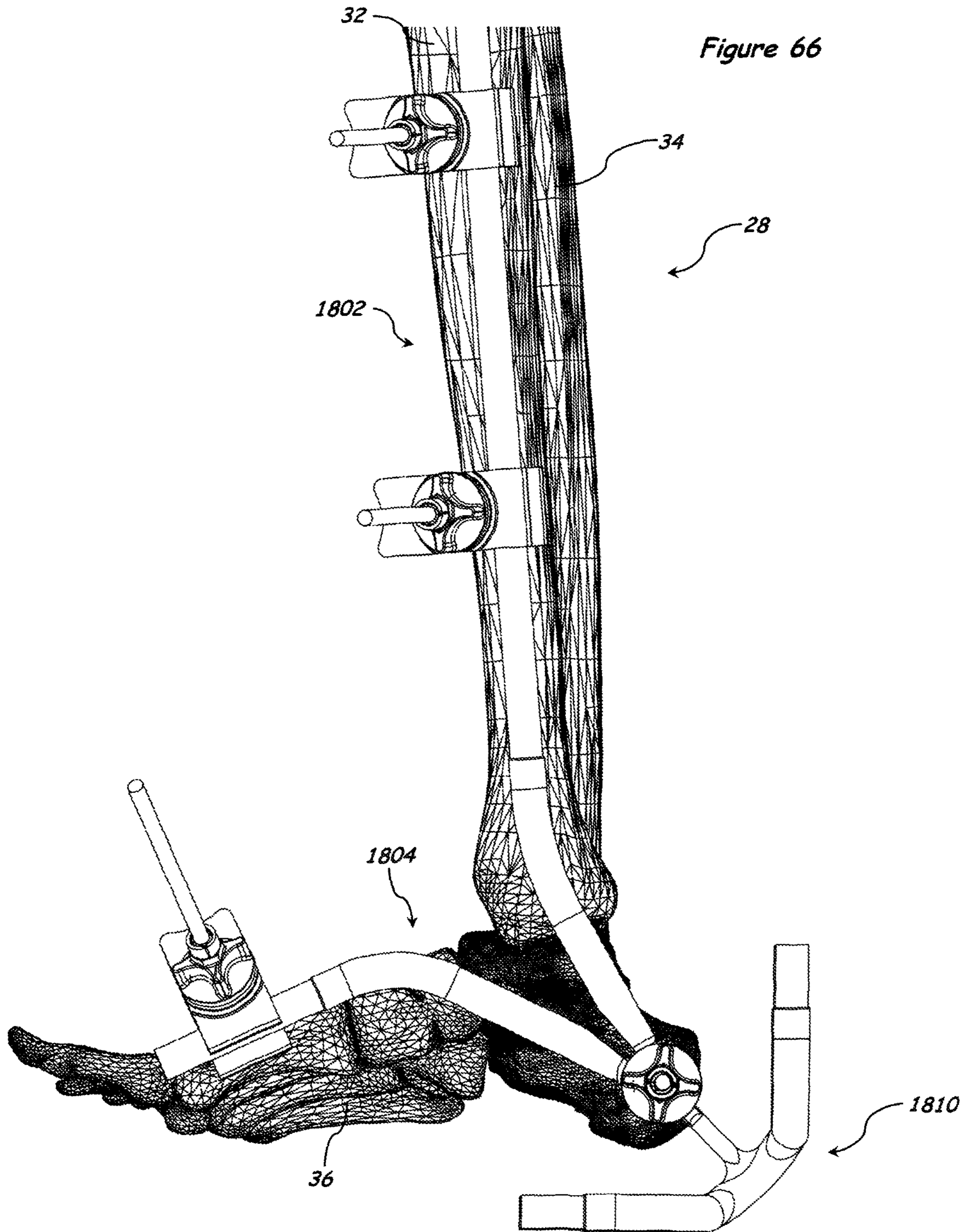


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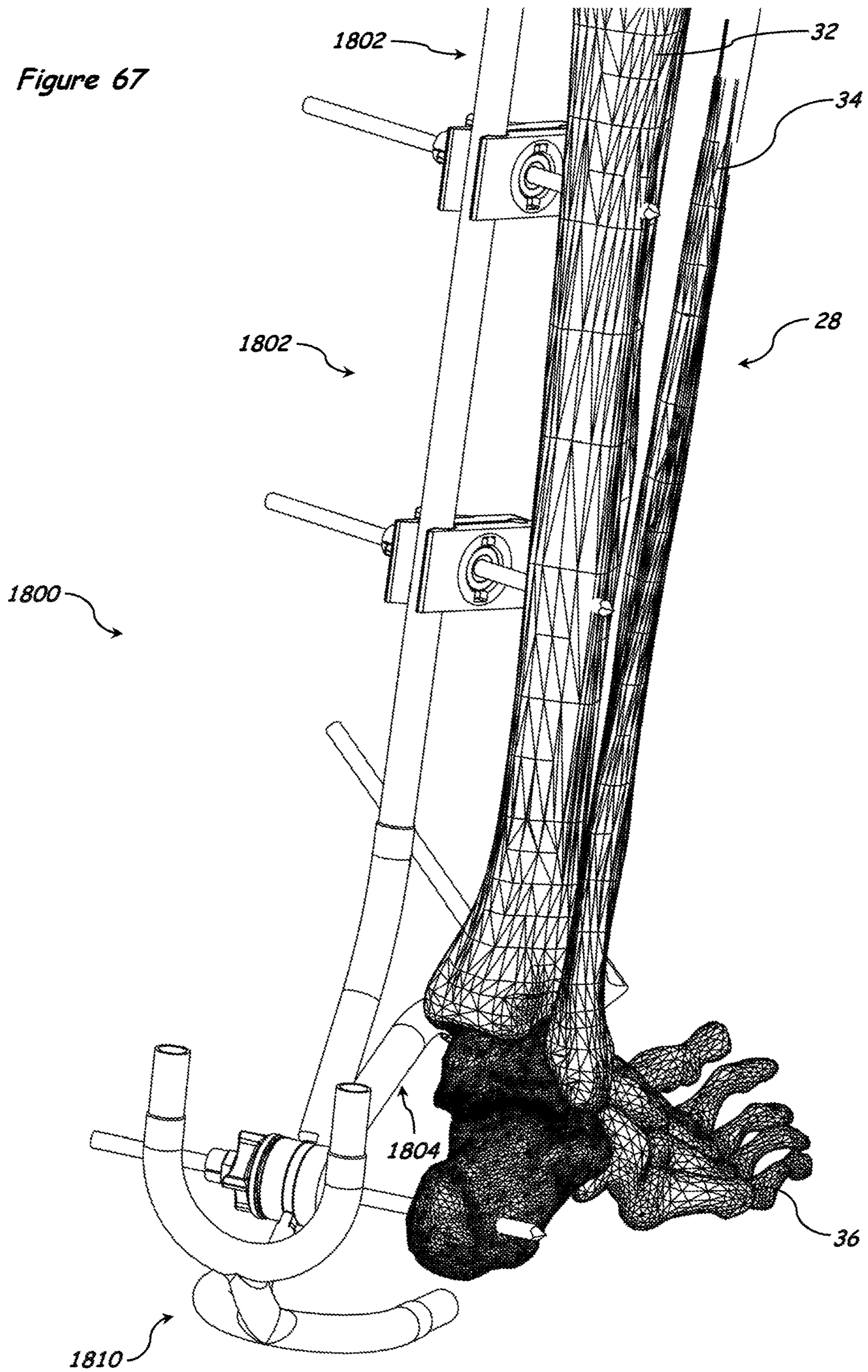


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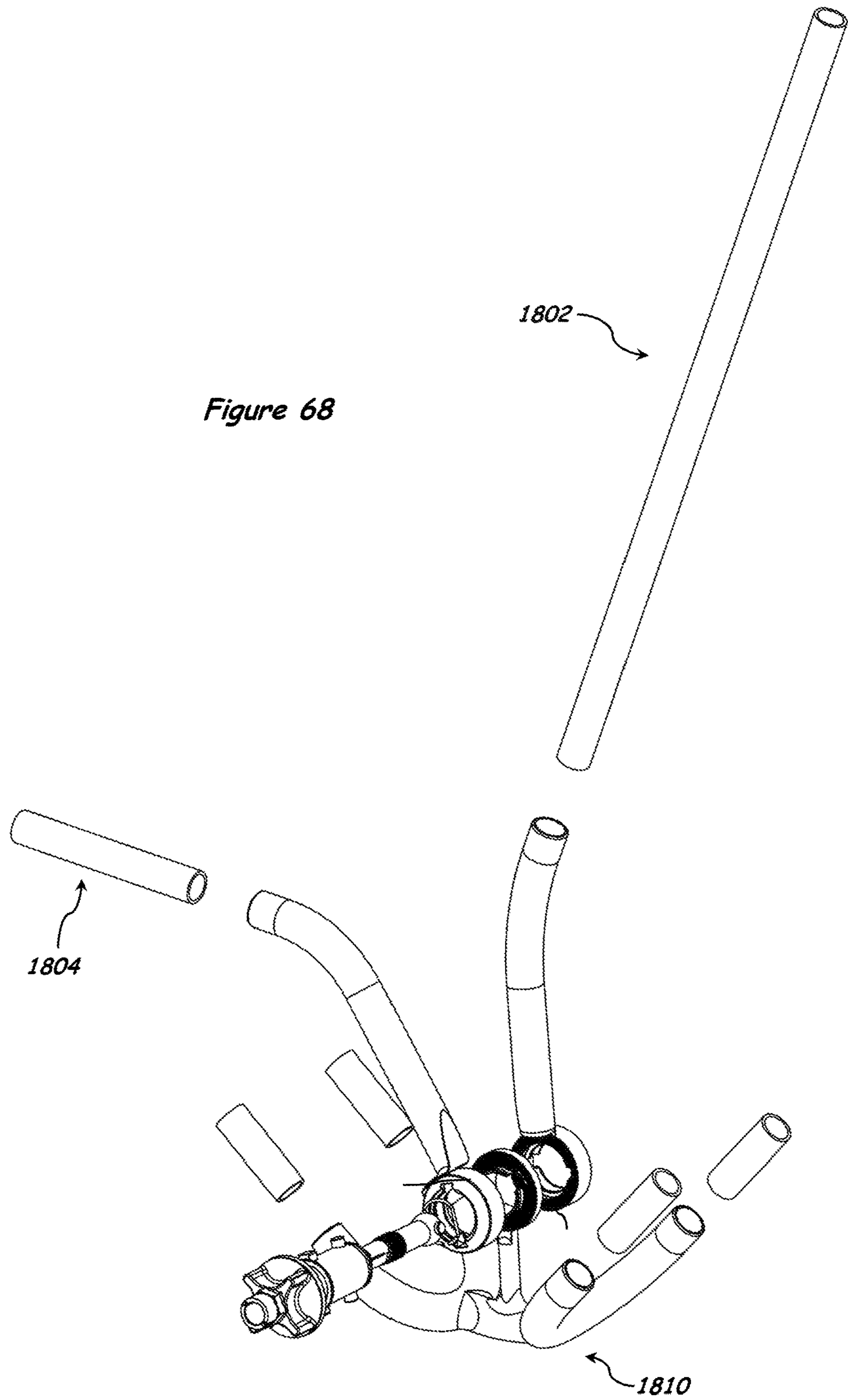
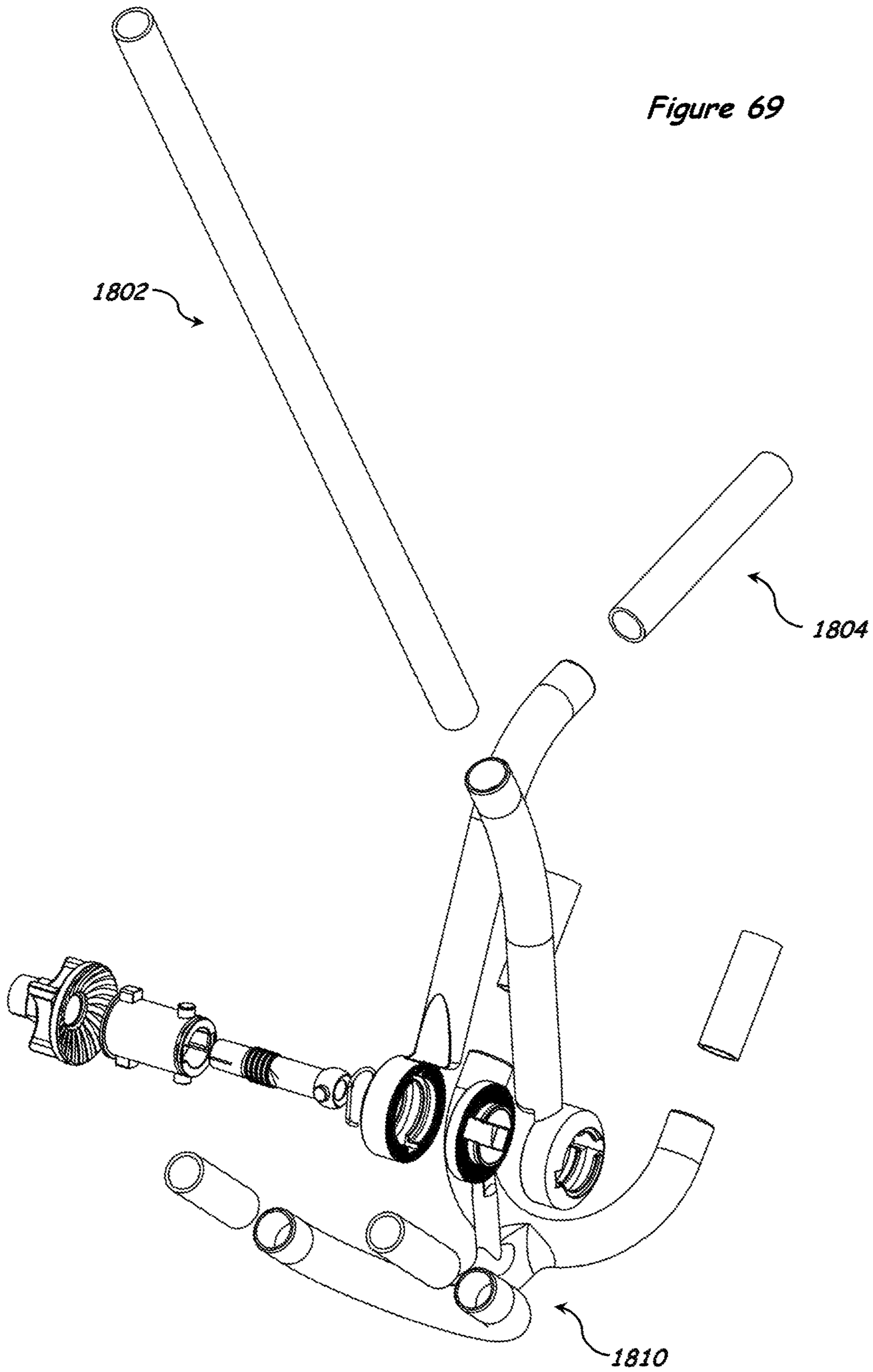


Figure 69





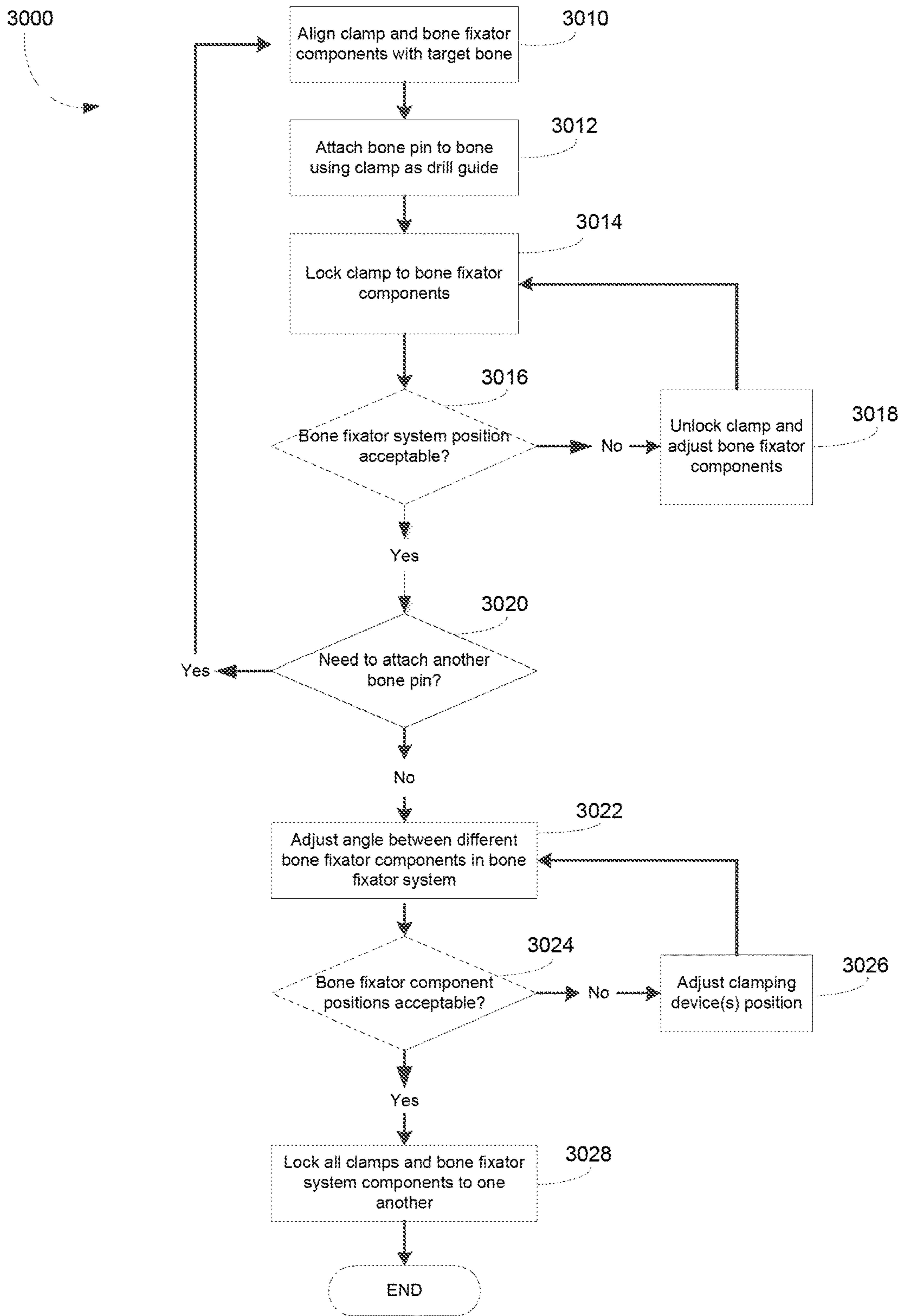


Figure 70

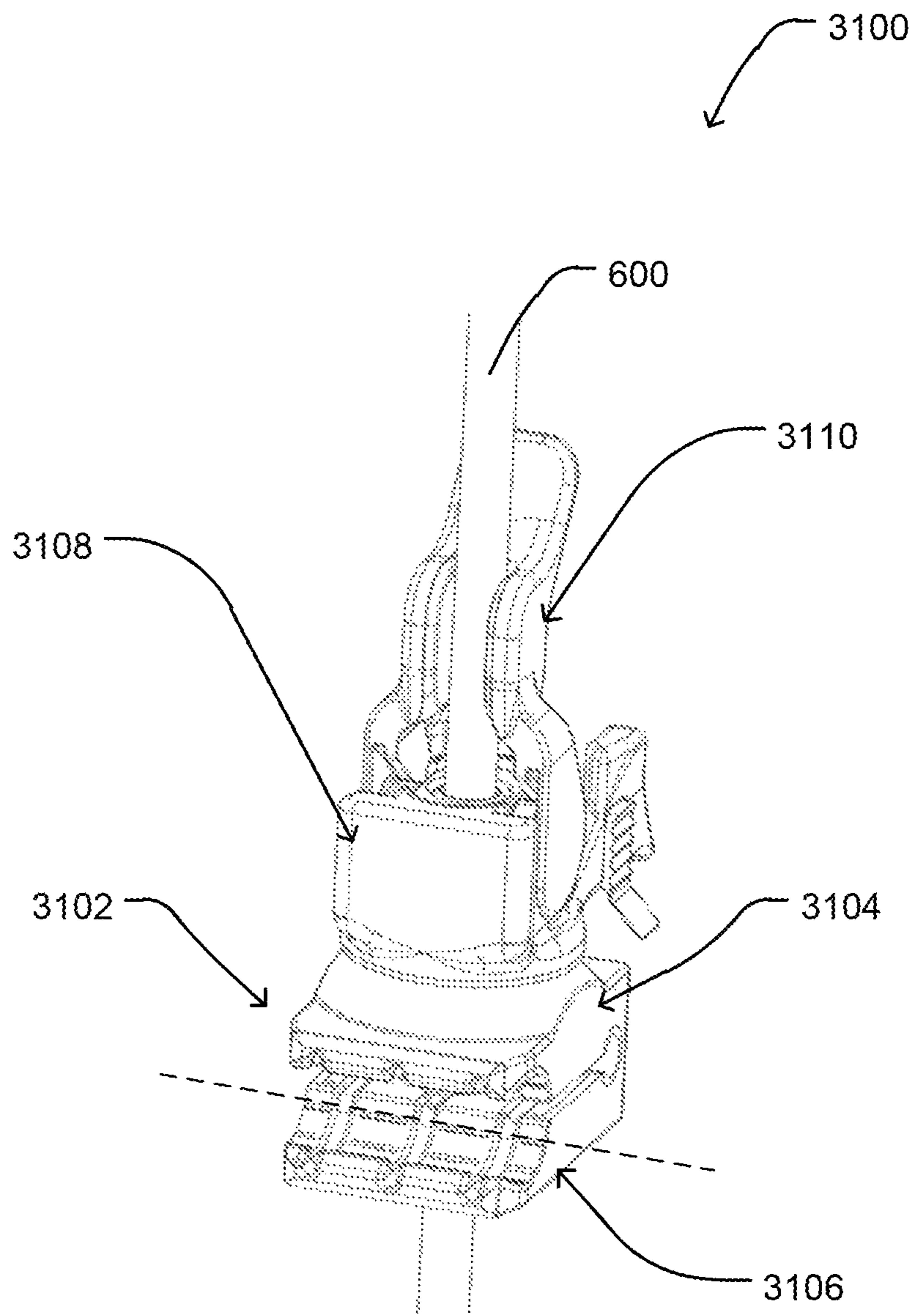


FIG. 71

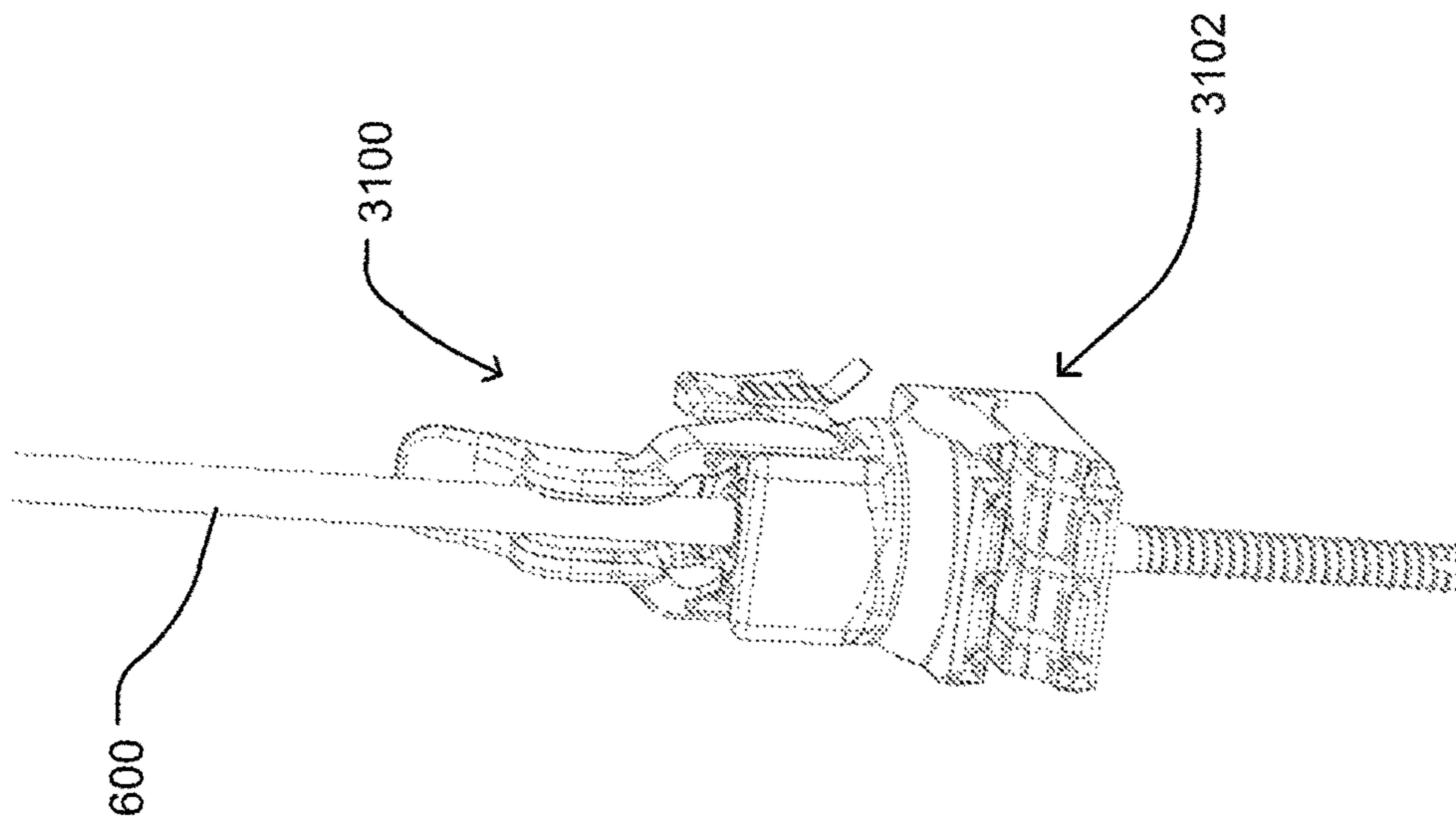


FIG. 72B

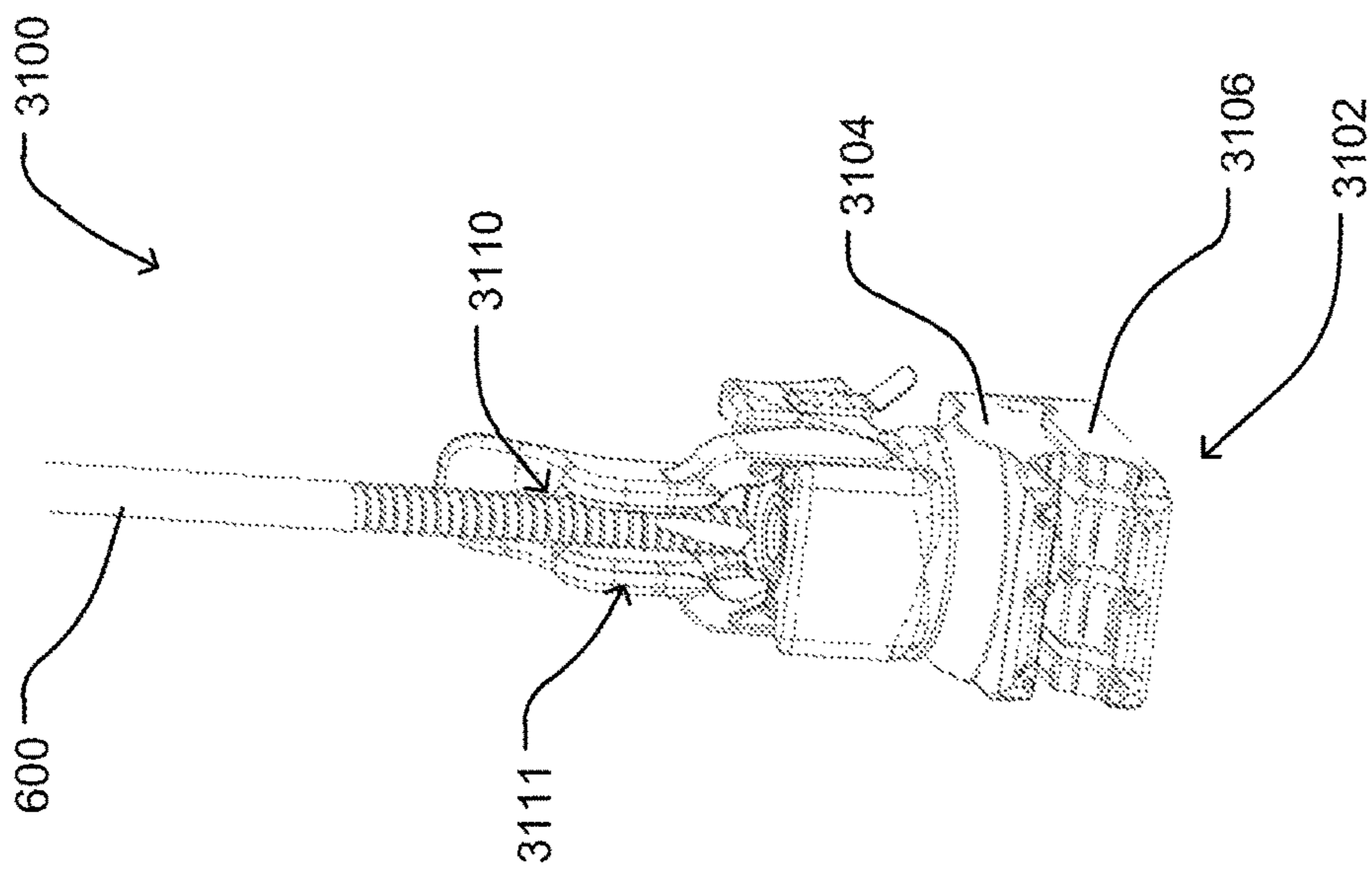


FIG. 72A

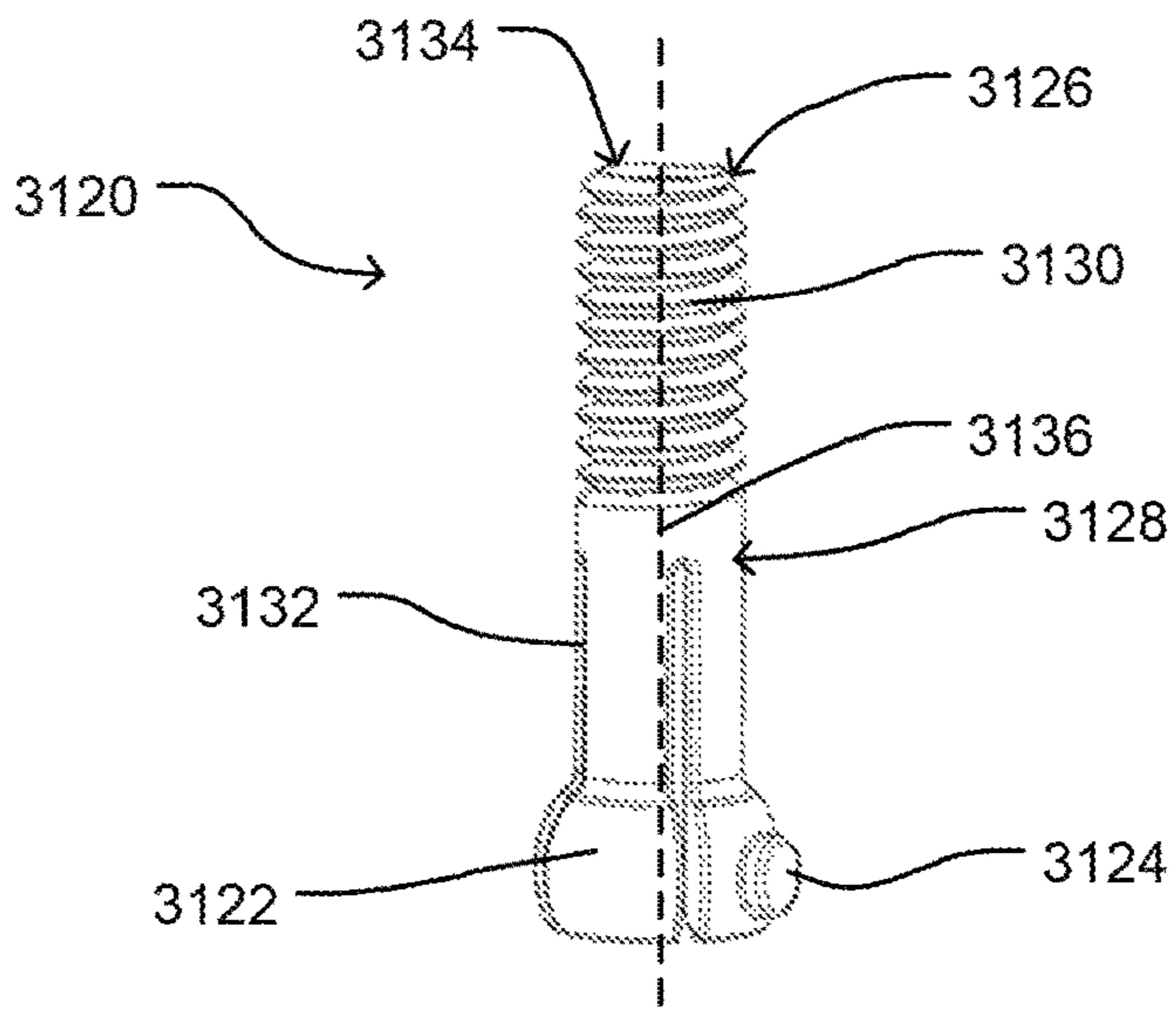


FIG. 73A

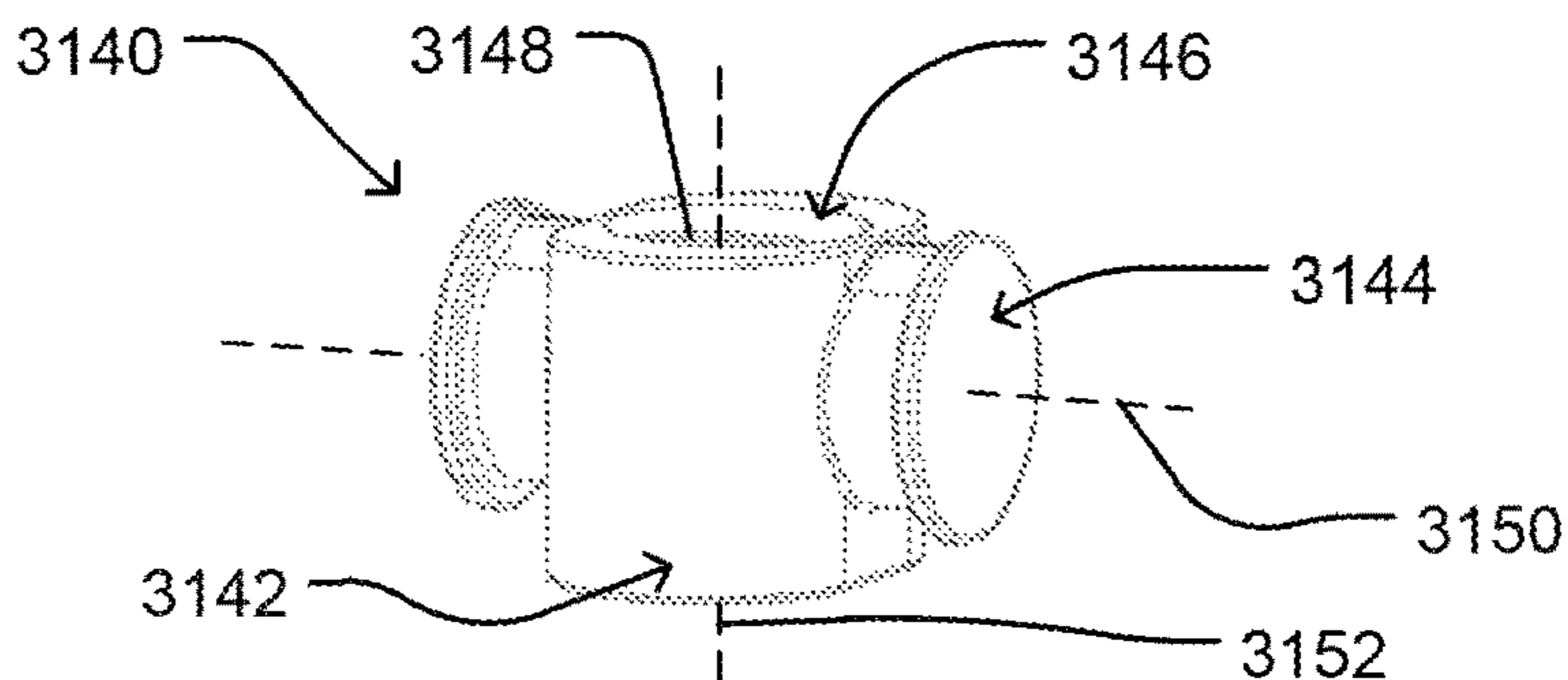


FIG. 73B

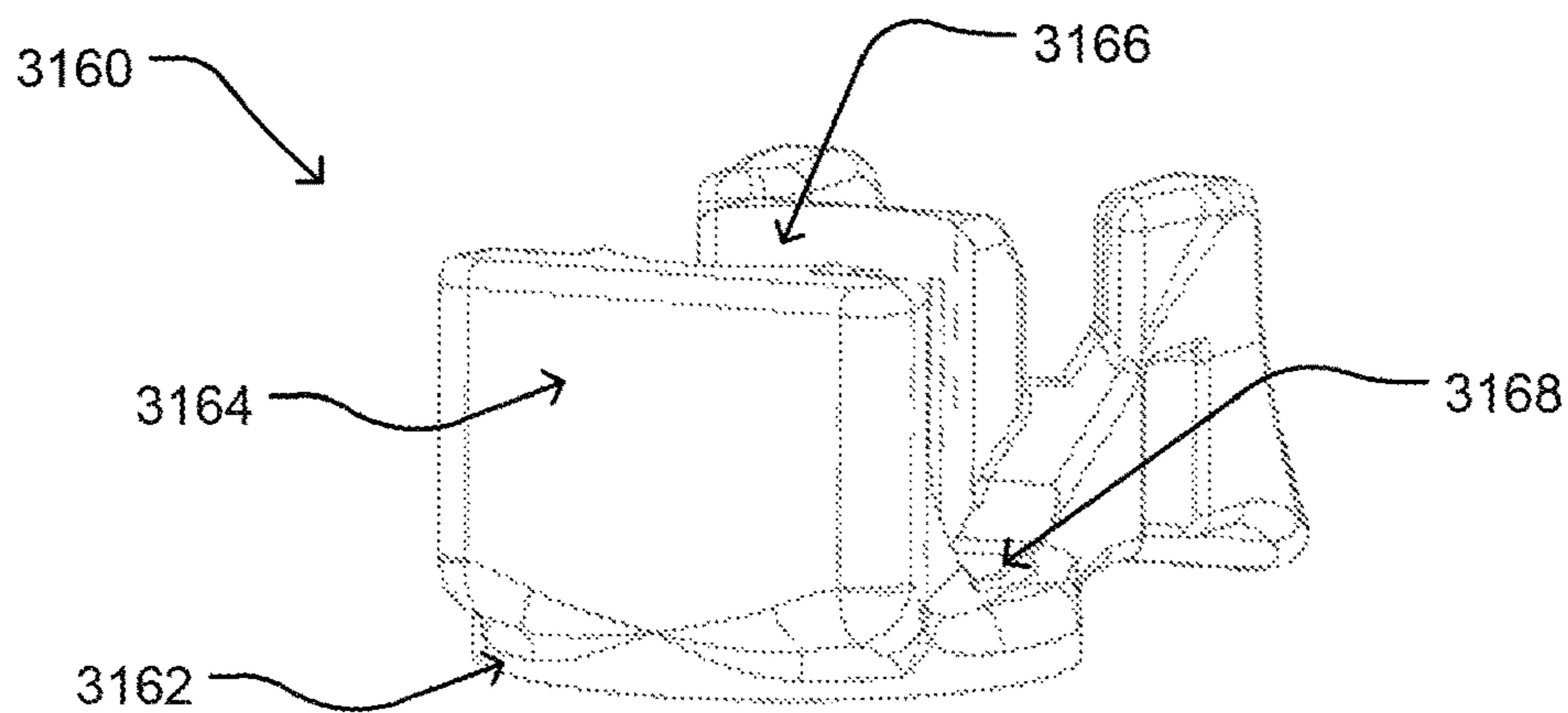


FIG. 73C

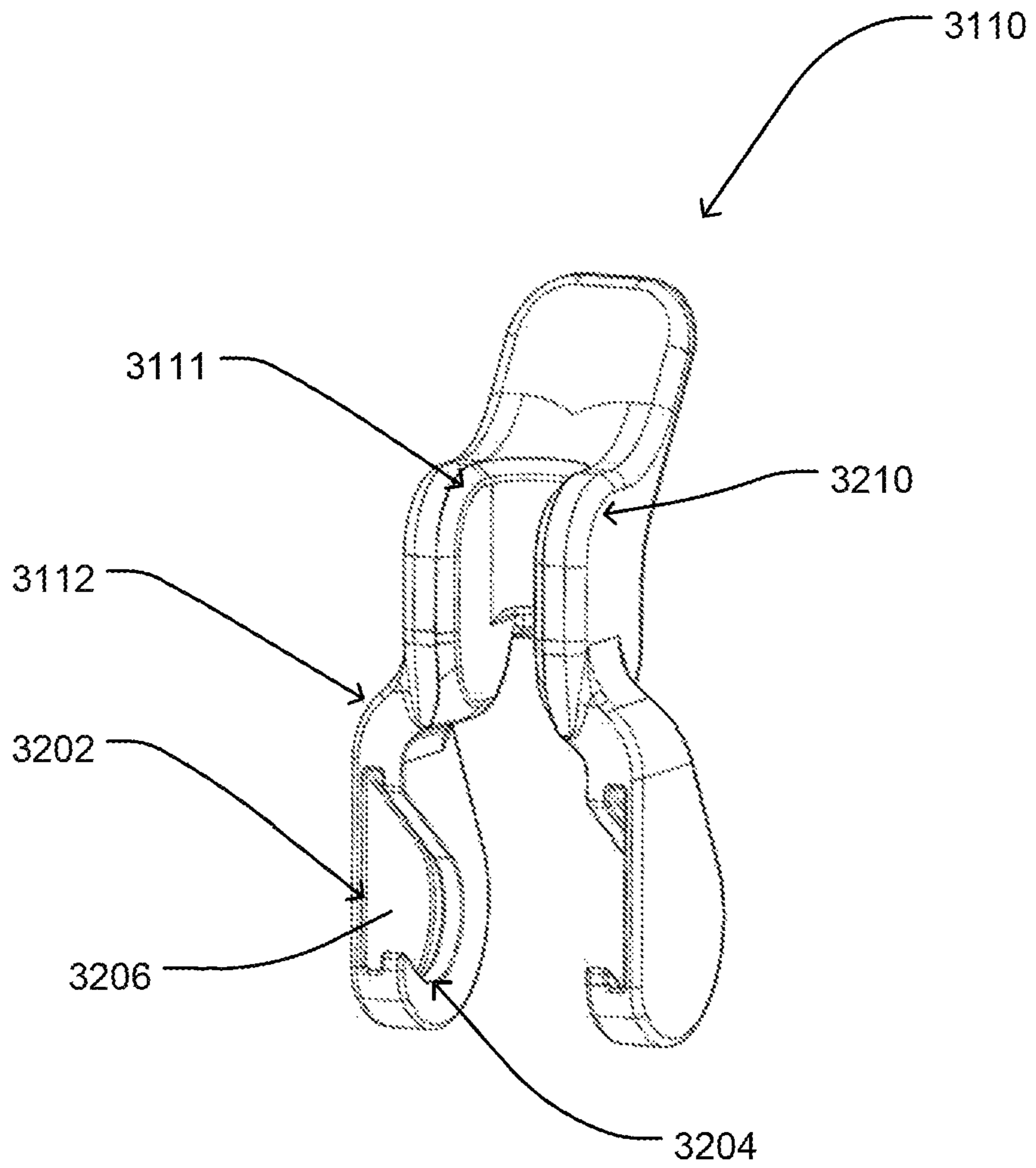


FIG. 73D

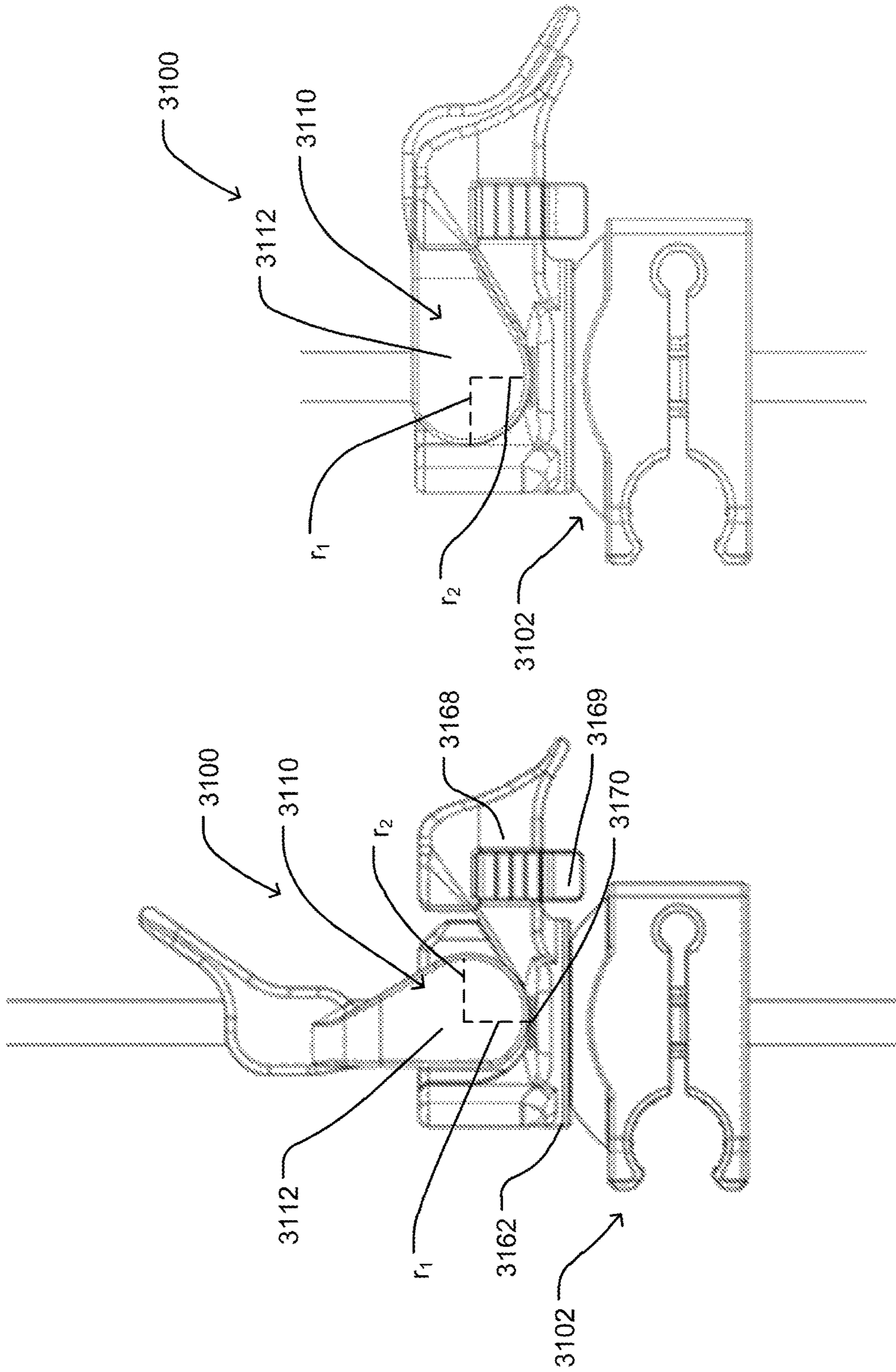


FIG. 74B

FIG. 74A

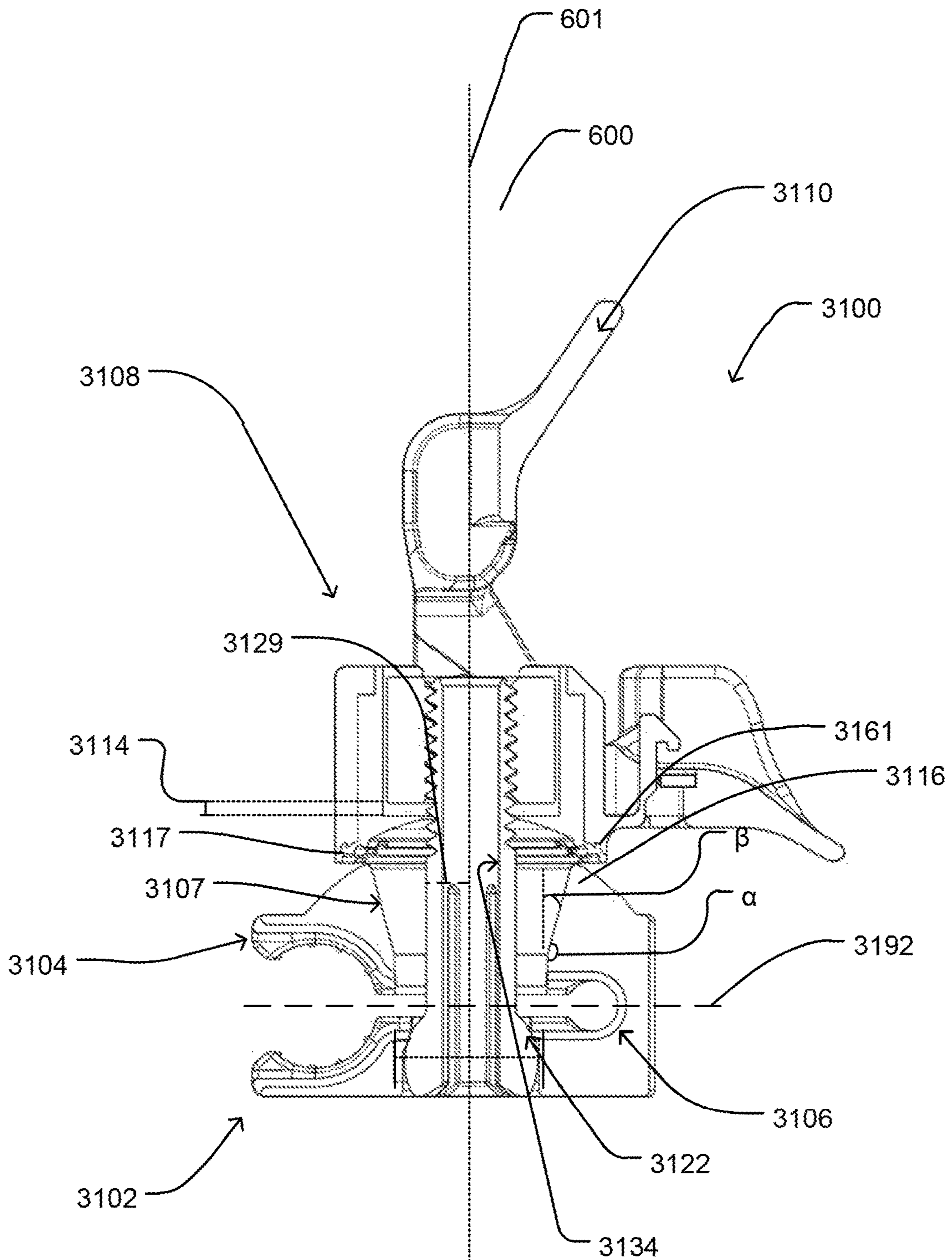


FIG. 75A

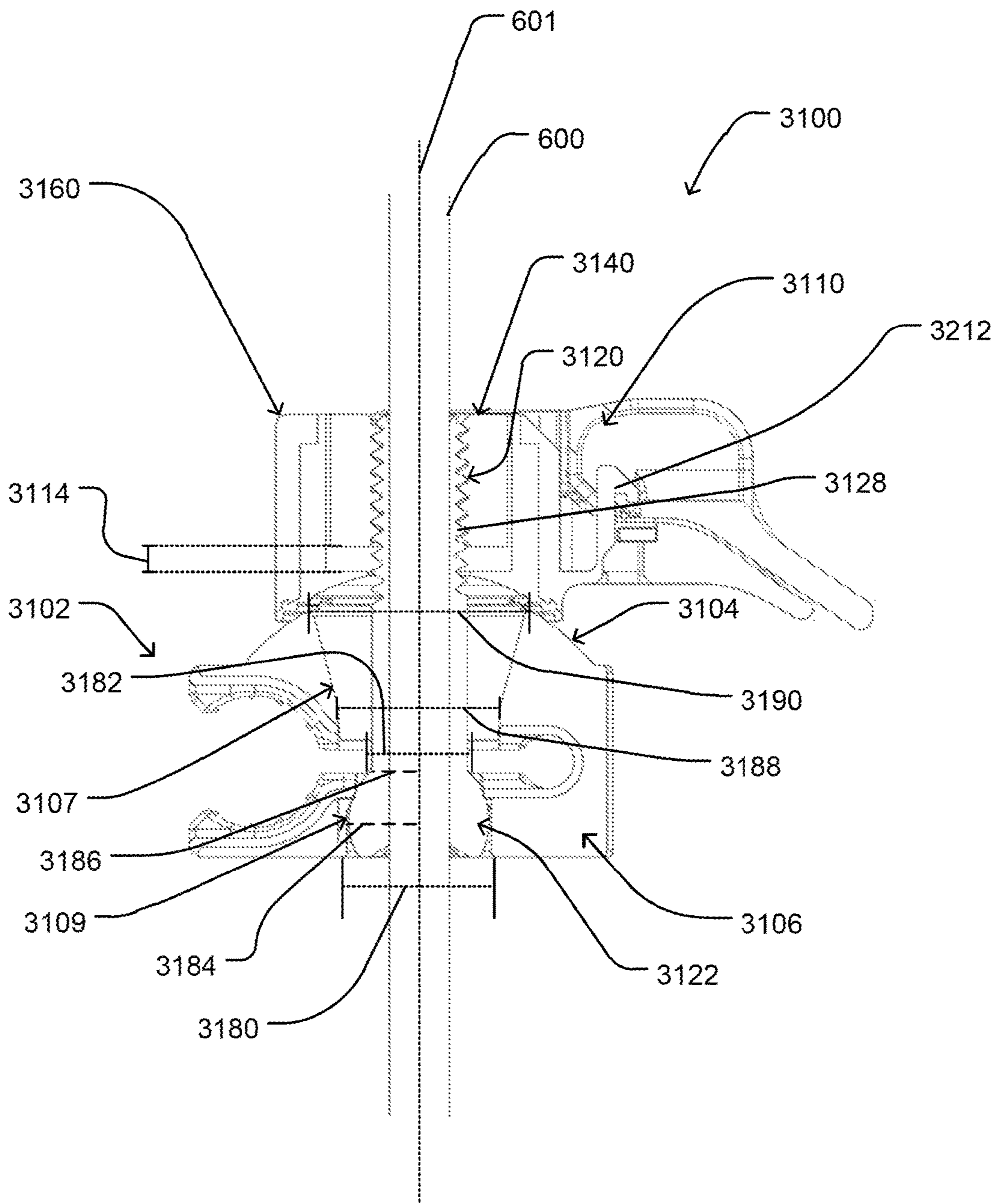


FIG. 75B



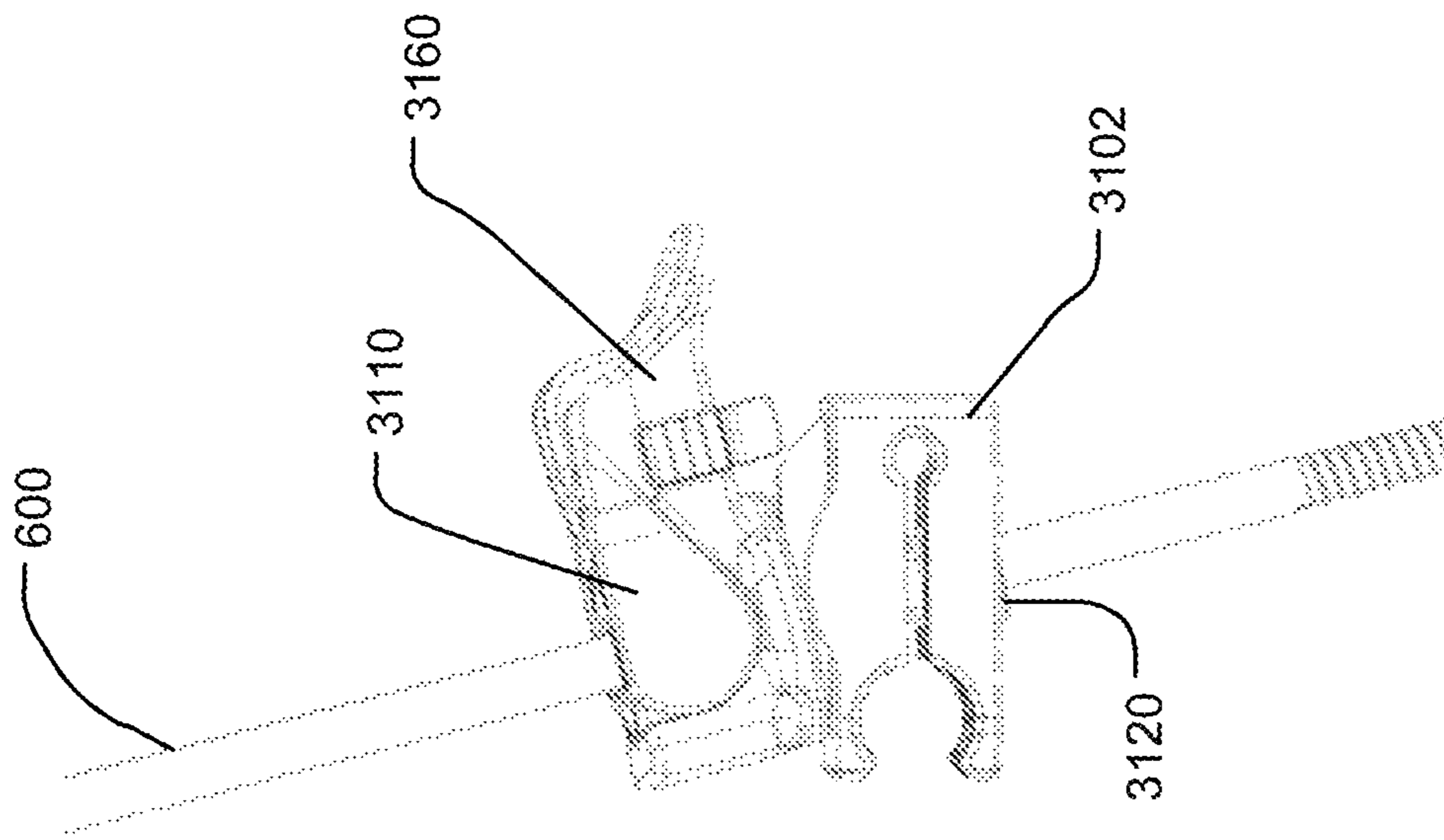


FIG. 76A

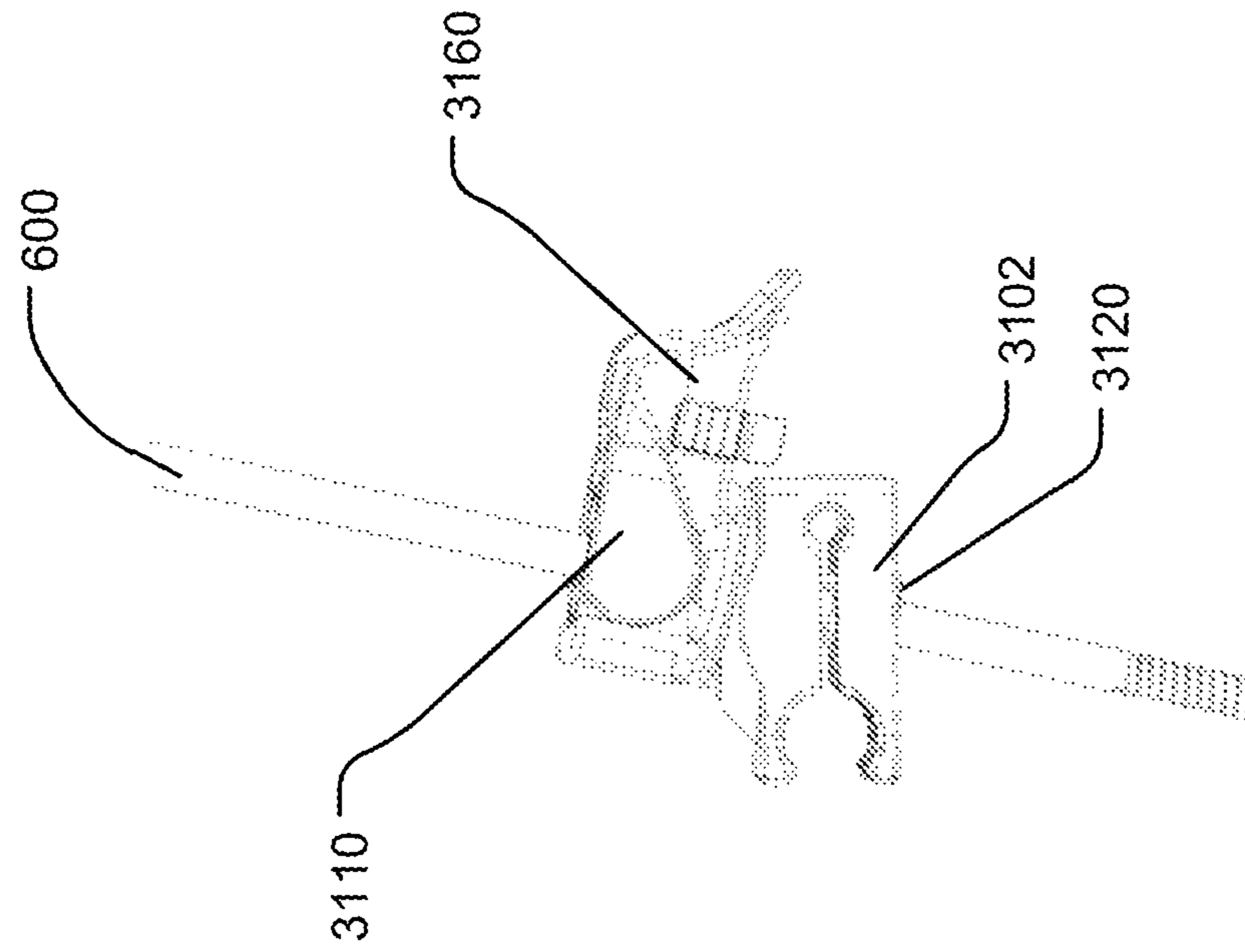


FIG. 76B

## CLAMPING DEVICE FOR USE WITH AN ANATOMIC EXTERNAL FIXATION DEVICE

### CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 15/359,479, entitled "CLAMPING DEVICE FOR USE WITH AN ANATOMIC EXTERNAL FIXATION DEVICE," filed Nov. 22, 2016, which is a continuation-in-part of U.S. patent application Ser. No. 14/871,618, entitled "CLAMPING DEVICE FOR USE WITH AN ANATOMIC EXTERNAL FIXATION SYSTEM," filed on Sep. 30, 2015, which claims priority to U.S. Application 62/058,262, entitled "Anatomic External Fixation Device," filed on Oct. 1, 2014, the disclosures of which are incorporated herein by reference in their entireties for all purposes.

### TECHNICAL FIELD

The present disclosure relates generally to fracture fixation systems, methods, and components. More particularly, the disclosure relates to improved anatomic external fixation systems, methods, and components. Particular embodiments described herein can be used to set bone fragments in long or flat bone fractures (e.g., tibia fractures, femur fractures, fibula fractures, pelvis fractures, etc. . . .).

### BACKGROUND

External fixation devices have been widely used in the treatment of long bone fractures and are best suited in cases of unstable, comminuted fractures. An example of this would be a compound fracture of the tibia that would generally be fixed with a cast. If the fracture is too comminuted, the cast will be unable to provide enough support to the fragments, thus leading to a malunion or a nonunion. The external fixation device helps stabilize the bone fragments and allow the patient a quicker recovery time with fewer complications.

Current external fixation devices consist of straight rods and ring-frames made of carbon fiber that can be interconnected through the use of clamps. The clamps can be two sided with one side clamping to the straight bar and the other side clamping to a bone pin that is fixed to a bone or bone fragment. These two clamps are connected to each other via a rotating joint that allows for some adjustability along one plane, thus allowing various angles in between the rods and the pins. Once the surgeon has adjusted the rods and pins to the desired positions, they have to lock everything in place by tightening nuts on each side of the clamp. The process of locking each clamp in place can be cumbersome and may require multiple assistants to aid in the procedure. This adds complexity and wastes valuable resources.

External fixator devices with hinges for fixing injury around joints such as the elbow, the knee, and the ankle are generally designed for use only on the right side or only on the left side of the joint or limb. These hinged systems must be mounted on the bone with the mechanical pivot axis of the device aligned with the natural pivot axis of the joint. These designed limitations not only demand that hospitals dedicate a large inventory for accommodating high volume of external fixator devices, but also increase surgical time and complexity in installing the devices on patients.

Therefore, a need exists for improved external fixation systems, methods, and components for use in fracture fixation.

## SUMMARY

The present disclosure provides components and systems for externally fixing and precisely adjusting fractures in general, and more particularly fractures in a bone or near a joint, such as fractures near the elbow, knee, and ankle. The components and systems according to some exemplary embodiments wherein the same system can be used on either the right side or the left side of a bone or joint. According to some other exemplary embodiments, a single system can be used across both sides of the bone or joint simultaneously. The systems and their components include unitary construction, unitary modular construction and modular construction.

According to an aspect of the present disclosure, a clamping device for an external fixation system includes a clamp body and a locking assembly. The clamp body includes a first jaw and a second jaw and defines a first channel configured to accommodate a fixation element along a longitudinal axis of the first channel. The first jaw defines a first opening and the second jaw defines a second opening. The locking assembly includes a first locking element, a second locking element, and a lever configured to couple to the second locking element. The first locking element includes a first end and a shaft portion extending from the first end. The shaft portion is sized to pass through the first opening and the second opening. The second opening is sized to restrict the first end from passing through the second opening. The first locking element defines a second channel sized to receive a bone pin. The locking assembly is configured to reduce a distance between the first jaw and the second jaw responsive to rotation of the second locking element relative to the first locking element. The lever is configured to attach to the second locking element and rotate about the second locking element from a first position to a second position to cause the distance between the first jaw and the second jaw to be reduced further while the first end is in contact with the second opening.

According to another aspect of the present disclosure, a clamping device for an external fixation system includes a clamp body and a locking assembly. The clamp body includes a first jaw and a second jaw. The first jaw defines a first opening and the second jaw defines a second opening. The locking assembly includes a first locking element, a second locking element, and a lever. The first locking element includes a first end and a shaft portion extending from the first end. The shaft portion is sized to pass through the first opening and the second opening. The lever is configured to be attached to the second locking element and rotated about the second locking element to cause a distance between the first jaw and the second jaw to be reduced while the first locking element is in contact with the second opening.

Some or all of the systems, components and subcomponents of the present invention can be single-use or disposable. Also some or all of the systems, components and subcomponents of the present invention can be made of a unitary construction (formed from a single piece of metal or material) or unitary modular construction (plurality of components and/or subcomponents permanently connected by standard means, such as injection molding, welding, or soldering), or of modular construction (plurality of components and/or subcomponents removably connected by standard means, such as threading or snap-fitting).

These and other features of various embodiments can be understood from a review of the following detailed description in conjunction with the accompanying drawings.

It is to be understood that both the foregoing general description and the following detailed description are exemplary and explanatory and are not restrictive of the present invention, as claimed.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a superior-lateral perspective view of an elbow with a first embodiment of the elbow external fixator and its associated clamps.

FIG. 2 is a superior-medial perspective view of an elbow with the first embodiment of the elbow external fixator and its associated clamps.

FIG. 3 is a superior perspective view of an elbow with the first embodiment of the elbow external fixator and its associated clamps.

FIG. 4 is a detailed anterior-medial exploded view of the first embodiment of the elbow external fixator.

FIG. 5 is a detailed anterior-lateral exploded view of the first embodiment of the elbow external fixator.

FIG. 6 is a perspective view of a first embodiment of a closed clamp that can be utilized in all the embodiments of the external fixator.

FIG. 6A is a cross-sectional view taken along the line 6A-6A of FIG. 6

FIG. 7 is a perspective view of a double diameter pin that can be utilized in the first embodiment of the closed clamp.

FIG. 8 is an exploded bottom perspective view of the first embodiment of the closed clamp that can be utilized in all the embodiments of the external fixator.

FIG. 9 is an exploded side view of the first embodiment of the closed clamp that can be utilized in all the embodiments of the external fixator.

FIG. 9A is a cross-sectional view taken along the line 9A-9A of FIG. 9

FIG. 10 is an exploded top perspective view of the first embodiment of the closed clamp that can be utilized in all the embodiments of the external fixator.

FIG. 11 is a perspective view of a first embodiment of an open clamp that can be utilized in all the embodiments of the external fixator.

FIG. 11A is a cross-sectional view taken along the line 11A-11A of FIG. 11

FIG. 12 is a perspective view of a double diameter pin used in the first embodiment of the open clamp.

FIG. 13 is an exploded top perspective view of the first embodiment of the open clamp that can be utilized in all the embodiments of the external fixator.

FIG. 14 is an exploded side view of the first embodiment of the open clamp that can be utilized in all the embodiments of the external fixator.

FIG. 15 is an exploded bottom perspective view of the first embodiment of the open clamp that can be utilized in all the embodiments of the external fixator.

FIG. 15A is a cross-sectional view of a second embodiment of the open clamp system that can be utilized in all the embodiments of the external fixator.

FIG. 15B is a cross-sectional view of the clamp body of FIG. 15A.

FIG. 15C is a side view of the shaft of FIG. 15A.

FIG. 15D is a cross-sectional view taken along the line 15D-15D of FIG. 15C.

FIG. 16 is a perspective view of a third embodiment of a multiple-part/multiple-material open clamp that can be utilized in all the embodiments of the external fixator.

FIG. 17 is an exploded perspective view of the third embodiment of the multiple-part/multiple-material open clamp that can be utilized in all the embodiments of the external fixator.

FIG. 17A is a cross-sectional view taken along the line 17A-17A of FIG. 17.

FIG. 18 is a lateral perspective view of an elbow with a second embodiment of the elbow external fixator and its associated clamps.

FIG. 19 is a superior-lateral perspective view of an elbow with the second embodiment of the elbow external fixator and its associated clamps.

FIG. 20 is a posterior-lateral perspective view of an elbow with the second embodiment of the elbow external fixator and its associated clamps.

FIG. 21 is a detailed posterior-lateral exploded view of the second embodiment of the elbow external fixator.

FIG. 21A is a cross-sectional view taken along the line 21A-21A of FIG. 21.

FIG. 21B is a cross-sectional view taken along the line 21B-21B of FIG. 21.

FIG. 22 is a detailed anterior-lateral exploded view of the second embodiment of the elbow external fixator.

FIG. 22A is a cross-sectional view taken along the line 22A-22A of FIG. 22.

FIG. 23 is an anterior perspective view of a leg with a first embodiment of the knee external fixator and its associated clamps.

FIG. 24 is an anterior-medial perspective view of a leg with the first embodiment of the knee external fixator and its associated clamps.

FIG. 25 is an anterior-lateral perspective view of a leg with the first embodiment of the knee external fixator and its associated clamps.

FIG. 26 is a detailed anterior-medial exploded view of the first embodiment of the knee external fixator.

FIG. 27 is a detailed anterior-lateral exploded view of the first embodiment of the knee external fixator.

FIG. 28 is an anterior perspective view of a leg with a second embodiment of the knee external fixator and its associated clamps.

FIG. 29 is an anterior-medial perspective view of a leg with the second embodiment of the knee external fixator and its associated clamps.

FIG. 30 is an anterior-lateral perspective view of a leg with the second embodiment of the knee external fixator and its associated clamps.

FIG. 31 is a detailed anterior-lateral exploded view of the second embodiment of the knee external fixator.

FIG. 32 is a detailed anterior-medial exploded view of the second embodiment of the knee external fixator.

FIG. 33 is an anterior perspective view of a leg with a third embodiment of the knee external fixator and its associated clamps.

FIG. 34 is a superior-medial perspective view of a leg with the third embodiment of the knee external fixator and its associated clamps.

FIG. 35 is a superior-lateral perspective view of a leg with the third embodiment of the knee external fixator and its associated clamps.

FIG. 36 is a detailed superior-lateral exploded view of the third embodiment of the knee external fixator.

FIG. 37 is a detailed superior-medial exploded view of the third embodiment of the knee external fixator.

FIG. 38 is a superior-medial perspective view of a leg with a fourth embodiment of the knee external fixator and its associated clamps.

## 5

FIG. 39 is a superior-lateral perspective view of a leg with the fourth embodiment of the knee external fixator and its associated clamps.

FIG. 40 is a detailed superior-medial exploded view of the fourth embodiment of the knee external fixator.

FIG. 41 is a detailed superior-lateral exploded view of the fourth embodiment of the knee external fixator.

FIG. 42 is an anterior-medial perspective view of a leg with a first embodiment of the ankle external fixator and its associated clamps.

FIG. 43 is an anterior-lateral perspective view of a leg with the first embodiment of the ankle external fixator and its associated clamps.

FIG. 44 is a posterior-lateral perspective view of a leg with the first embodiment of the ankle external fixator and its associated clamps.

FIG. 45 is an anterior-medial perspective view of a leg with a second embodiment of the ankle external fixator and its associated clamps.

FIG. 46 is an anterior-lateral perspective view of a leg with the second embodiment of the ankle external fixator and its associated clamps.

FIG. 47 is a posterior-medial perspective view of a leg with the second embodiment of the ankle external fixator and its associated clamps.

FIG. 48 is an anterior-medial perspective view of a leg with a third embodiment of the ankle external fixator and its associated clamps.

FIG. 49 is a medial perspective view of a leg with the third embodiment of the ankle external fixator and its associated clamps.

FIG. 50 is a posterior-lateral perspective view of a leg with the third embodiment of the ankle external fixator and its associated clamps.

FIG. 51 is a detailed posterior-lateral exploded view of the third embodiment of the ankle external fixator.

FIG. 52 is a detailed posterior-medial exploded view of the third embodiment of the ankle external fixator.

FIG. 53 is an anterior-medial perspective view of a leg with a fourth embodiment of the ankle external fixator and its associated clamps.

FIG. 54 is a medial perspective view of a leg with the fourth embodiment of the ankle external fixator and its associated clamps.

FIG. 55 is a posterior-lateral perspective view of a leg with the fourth embodiment of the ankle external fixator and its associated clamps.

FIG. 56 is a detailed posterior-lateral view of the fourth embodiment of the ankle external fixator.

FIG. 57 is a detailed medial view of the fourth embodiment of the ankle external fixator.

FIG. 58 is a detailed posterior-lateral exploded view of the fourth embodiment of the ankle external fixator.

FIG. 59 is a detailed posterior-medial exploded view of the fourth embodiment of the ankle external fixator.

FIG. 60 is a detailed exploded view of the cartridge utilized in the fourth embodiment of the ankle external fixator.

FIG. 61 is a section view of the main body of the cartridge utilized in the fourth embodiment of the ankle external fixator.

FIG. 62 is an anterior-medial perspective view of a leg with a fifth embodiment of the ankle external fixator and its associated clamps.

FIG. 63 is a medial perspective view of a leg with the fifth embodiment of the ankle external fixator and its associated clamps.

## 6

FIG. 64 is a posterior-inferior perspective view of a leg with the fifth embodiment of the ankle external fixator and its associated clamps.

FIG. 65 is an anterior-medial perspective view of a leg with a sixth embodiment of the ankle external fixator and its associated clamps.

FIG. 66 is a medial perspective view of a leg with the sixth embodiment of the ankle external fixator and its associated clamps.

FIG. 67 is a posterior-lateral perspective view of a leg with the sixth embodiment of the ankle external fixator and its associated clamps.

FIG. 68 is a detailed posterior-medial exploded view of the sixth embodiment of the ankle external fixator.

FIG. 69 is a detailed posterior-lateral exploded view of the sixth embodiment of the ankle external fixator.

FIG. 70 is a flow diagram of a method of fixating a bone fixator system to a target joint of a subject.

FIG. 71 is a perspective view of an embodiment of a clamping device.

FIG. 72A is perspective view of an embodiment of a bone pin to be received in the clamping device of FIG. 71.

FIG. 72B is a perspective view of an embodiment of a bone pin that is received in the clamping device of FIG. 71.

FIG. 73A is a perspective view of an embodiment of a locking element of a locking assembly of the clamping device of FIG. 71.

FIG. 73B is a perspective view of an embodiment of another locking element of the clamping device of FIG. 71.

FIG. 73C is a perspective view of an embodiment of another locking element of the clamping device of FIG. 71.

FIG. 73D is a perspective view of an embodiment of a lever of the clamping device of FIG. 71.

FIG. 74A is a side view of an embodiment of the clamping device of FIG. 71 in which the lever is in a first position.

FIG. 74B is a side view of an embodiment of the clamping device of FIG. 71 in which the lever is in a second position.

FIG. 75A is a cross section view of an embodiment of the clamping device of FIG. 71 in which the lever is in the first position.

FIG. 75B is a cross section view of an embodiment of the clamping device of FIG. 71 in which the lever is in the second position.

FIG. 76A is a side view of an embodiment of the clamping device of FIG. 71 in which the bone pin is secured in a first orientation.

FIG. 76B is a side view of an embodiment of the clamping device of FIG. 71 in which the bone pin is secured in a second orientation.

## DETAILED DESCRIPTION

The following detailed description and the appended drawings describe and illustrate various exemplary external fixation systems, methods, and components. The description and drawings are exemplary in nature and are provided to enable one skilled in the art to make and use one or more exemplary external fixation systems and/or components, and/or practice one or more exemplary methods. They are not intended to limit the scope of the claims in any manner.

The use of “e.g.,” “etc.,” “for instance,” “in example,” and “or” and grammatically related terms indicates non-exclusive alternatives without limitation, unless otherwise noted. The use of “optionally” and grammatically related terms means that the subsequently described element, event, feature, or circumstance may or may not be present/occur, and that the description includes instances where said element,

event, feature, or circumstance occurs and instances where it does not. The use of “exemplary” refers to “an example of” and is not intended to convey a meaning of an ideal or preferred embodiment. The use of “attached” and “coupled” grammatically related terms refers to the fixed, releasable, or integrated association of two or more elements and/or devices with or without one or more other elements in between. Thus, the term “attached” or “coupled” and grammatically related terms includes releasably attaching or fixedly attaching two or more elements and/or devices in the present or absence of one or more other elements in between. As used herein, the terms “proximal” and “distal” are used to describe opposing axial ends of the particular elements or features being described in relation to anatomical placement. As used herein, the terms “proximal,” “distal,” “inferior,” “posterior,” and any other relative position terms are intended to facilitate clarity regarding the disclosed embodiments, and do not limit the disclosure to any particular frame of reference.

While the systems, methods, and components described herein are exemplified by systems and methods for external fixation of bones, the systems, methods, and components described and illustrated herein can be used to treat any suitable ailment or joint within the body of an animal, including, but not limited to, humans. Skilled artisans will be able to select a suitable ailment and/or joint within the body of an animal to utilize a system and/or method described herein according to a particular embodiment based on various considerations, including the type of ailment and/or the structural arrangement at a treatment site. Example joints considered suitable to utilize a system, method, and/or component described herein include, but are not limited to, the elbow joint, the knee joint, and the ankle joint.

#### A. External Fixation Systems and Clamping Systems

In some embodiments, components disclosed herein may be disposed in a substantially perpendicular orientation (e.g., having longitudinal axes that are less than 20 degrees from 90 degrees apart, less than 10 degrees from 90 degrees apart, less than 5 degrees from 90 degrees apart, less than 1 degree from 90 degrees apart, etc.). In some embodiments, components disclosed herein may be disposed in a substantially coplanar (e.g., being disposed in planes that are less than 20 degrees from coplanar, less than 10 degrees from coplanar, less than 5 degrees from coplanar, less than 1 degree from coplanar, etc.).

FIGS. 1-3 illustrate an exemplary human elbow 10 comprising a humerus 12, ulna 14, and radius 16 and one embodiment of an exemplary elbow-spanning external fixation system 100.

FIGS. 1-5 illustrate a first embodiment of an exemplary elbow-spanning external fixation system 100 comprising a first external fixation component 102, a second external fixation component 104, a fastener or locking means 106, a closed-end clamp system 300 and an open-end clamp system 400. The first external fixation component 102 can be adapted to attach to the humerus 12, the ulna 14 and/or the radius 16 by use of the closed-end clamp system 300 and/or open-end clamp system 400. The second external fixation component 104 can be adapted to attach to the humerus 12, the ulna 14 and/or the radius 16 by use of the closed-end clamp system 300 and/or open-end clamp system 400.

The first external fixation component 102, second external fixation component 104, fastener 106, closed-end clamp system 300 and open-end clamp systems 400 and 500 (shown in FIGS. 16-17) can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque

and/or other forces that may be applied to the system 100, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made biocompatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form a first external fixation component, a second external fixation component, a fastener, a closed-end clamp system and an open-end clamp system of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

In the illustrated embodiment 100 shown in FIGS. 1-5, the first external fixation component 102 comprises a first component proximal (e.g., first) end portion 108 and a first component distal (e.g., second) end portion 110. At least a portion of the first component proximal end portion 108 and at least a portion of the first component distal end portion 110 can be straight or curved. The first component distal end portion 110 includes a pivot structure 122 having a rough surface 124 and a through-bore having a circular cross-sectional shape for receiving a fastener such as fastener 106. The second external fixation component 104 comprises a second component proximal (e.g., first) end portion 112 and a second component distal (e.g., second) end portion 114. At least a portion of the second component proximal end portion 112 can be straight or curved. The second component proximal end portion 112 also includes a pivot structure 126 having a rough surface 128 and a threaded through-bore 132 having a circular cross-sectional shape for receiving a fastener such as fastener 106. The first external fixation component 102 and second external fixation component 104 are coupled and locked via a locking means such as a fastener 106 having a head 116 and at least a portion of its shaft threaded 120. The fastener 106 is configured to extend through the through-bore of the first pivot structure 122 and the threaded through-bore of the second pivot structure 126 to form a threaded connection with the second pivot structure 126 to form a movable hinge, articulator or mechanical joint 130. The hinge 130 is then locked in position by further tightening the fastener 106 which then interlocks the rough surface 124 of the first pivot structure 122 with the rough surface 128 of the second pivot structure 126. The interlocking or engagement of the rough surfaces 124 and 128 prevents the first and second external components 102 and 104 from rotating relatively to each other in a locking state.

Each of the first and second external fixation components 102 and 104 including their respective pivot structures 122 and 126 can be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy). The first and second external fixation components 102 and 104 each can have any cross-sectional shape including circular, and non-circular such as oval, square, rectangle, triangle, or any polygonal shapes, and the cross-sectional shape can be different along the length of each component (e.g. semi-circle, circle). Each of the first and second external fixation components 102 and 104 can have uniform or varying

diameter or thickness along its length. The first external fixation component **102** can be dimensioned and/or shaped to be the same or different from the second external fixation component **104**.

The pivot structures **122** and **126** can be integrally formed or permanently attached by standard means such as welding or soldering or gluing, or removably coupled by standard means such as threading or snap-fitting, to any locations along the length of their respective first and second external fixation components **102** and **104** including the portion disposed between the distal end portion and the proximal end portion of each external fixation components **102** and **104**. The pivot structures **122** and **126** can have any cross-sectional shape including circular, and non-circular such as oval, square, rectangle, triangle, or any polygonal shape. The length of each of the pivot structures **122** and **126** as measured along its axis of rotation or mechanical pivot axis X can be the same or different from the diameter or thickness of their respective first and second external fixation components **102** and **104**. The end surfaces **124** and **128** of pivot structures **122** and **126** comprising the rough surface each lies in a plane perpendicularly intersecting the mechanical pivot axis, but can also lie in a plane intersecting the mechanical pivot axis at an angle other than 90 degrees. The rough surfaces **124** and **128** can include serration or radial interdigitation or other irregularly shaped features which provide friction enhancement or anti-rotation to the fixation components in a locking state. One skilled in the art may choose to have the rough surfaces be disposed on an outer surface of one of the first and second pivot structures **122** and **126** and on an inner surface of the other of the first and second pivot structures **122** and **126** to provide anti-rotation. The rough surfaces can also be provided as separate inserts coupled to the pivot structures **122** and **126**. The pivot structures **122** and **126** can be an integral part of their respective external fixation components **102** or **104** or can be formed separately and assembled together later by welding, soldering or threading, for example. The pivot structures **122** and **126** each can be made of a unitary structure, a unitary modular or multi-component structure, or modular structure. An example of a modular pivot structure may include a pivot structure **122** or **126** having a non-circular cross-sectional shaped through-bore for receiving an insert having a matching, non-circular cross-sectional shape and a circular cross-sectional shaped through-bore with or without threads.

The locking means, such as fastener **106**, comprises an enlarged structure, such as a head **116**, with secure gripping surface features or geometry **118** for ease of handling the fastener during surgery, and a shaft **120** having engagement features such as threads which establish a threaded connection with the threaded through-bore **132** of the pivot structure **126** in the second external fixation component **104** during coupling and locking the external fixation components. The engagement features on the shaft can also include fins, protrusions or other fastening features known to one skilled in the art. The fastener **106** can also be a unitary, unitary modular or modular structure. An example of a modular fastener include a fastener as described but without the engagement features on its shaft, and a sleeve having engagement features on its outer surface adapted to cover the shaft of the fastener. The locking means can also include a first fastener such as fastener **106** and a second fastener such as a threaded nut. In this exemplary dual fastener system, both pivot structures **122** and **126** can have through-bores without threads or any engagement features, and arranged between the head of the first fastener and the nut. As the first fastener **106** or the second fastener (the threaded

nut) is tightened down, the external fixation components **102** and **104** are coupled and locked in position.

FIGS. **6-15** describe various embodiments of a novel bone clamp configured to provide simple locking of various fixation elements such as wires, pins, rods and bars simultaneously. These clamping devices as described below can be used with the external fixation systems of the present invention to couple to bones, or with any existing or commercialized external fixation systems.

FIGS. **6-10** show an embodiment of a closed-end clamp system **300** comprising a clamp body **302**, a knob **304** and a shaft **306**. The clamp body **302** having an open end **302c** and a close or hinged end **302d** connecting an upper jaw **302a** to a lower jaw **302b** forming a groove or aperture **308** for receiving an external fixation element such as the first or second external fixation components **102** and **104**, and a slot or spacing **310** in communication with the aperture **308**. Each of the upper and lower jaws **302a** and **302b** have a through-bore **000** formed in alignment and configured for receiving and operatively interacting with at least a portion of a locking element or locking assembly such as the shaft **306** configured for operably interacting with the knob **304** for locking the clamp system **300**.

The knob **304** comprises a knob body **304a** having a clamp body facing end **304b** and an opposing end **304c** and a through-bore dimensioned for receiving and operatively interacting with a shaft, such as shaft **306**, and extending longitudinally from the clamp body facing end **304b** to the opposing end **304c**. The knob body **304a** includes a funnel-like or frusto-conical internal surface **304e** or an internal surface having one of more tapered facets to guide, receive and alternatively compress and release a slit end, or a funnel-like or tapered external surface, of a shaft such as the shaft **306** for clamping a fixation element such as bone pin **600**. The funnel-like or frusto-conical internal surface **304e**, or more generally the through-bore bound by walls extending from the clamp body facing end **304b** to the opposing end **304c** of the knob body **304a**, is designed to be larger toward the clamp body facing end **304b** than toward the opposing end **304c** of the knob body **304a**, and includes a first locking feature such as threads **350**. The tapered internal surface **304e** can also be an insert. The through-bore **002** or opening in the opposing end **304c** of the knob **304** has a diameter smaller than the uncompressed diameter of the slit end **324** of the shaft **306** to provide interference fit among the inner surface **304e** of the knob **304**, the slit end **324** and the bone pin such as bone pin **600**. The opposing end **304c** of the knob body **304a** can include one or more slits **426a** or breakable lines as shown in FIG. **11A** for accommodating a broader range of dimensional tolerances of the bone pin **600** or **700**. The knob **304** can have irregularly shaped geometry **314** for providing a secure grip surface and optionally a hexagonally shaped geometry **316** that interfaces with a wrench.

The variable position shaft or shaft **306** includes an elongated body with a through-bore extending longitudinally along its length and dimensioned for receiving a fixation element, such as a bone pin **600** or **700**, an end portion including a stopper or an enlarged structure or structures, such as head **318**, which operatively interacts with at least a portion of an internal surface of one of said upper and lower jaws, such as jaws **302a** and **302b**, for preventing the shaft **306** from passing completely through the clamp body **302** or through the jaw **302a** or **302b**, which the stopper **318** first comes in contact with, and a locking or engagement feature such as threads **322** on the external surface of the shaft **306**, and one or more breakable lines or

slits 324 on an opposing end portion of the shaft. The slits 324 can also be disposed on the stopper 318 to provide similar compression onto the bone pin 600 or 700 during locking as shown in alternative embodiments of this invention. The tapered internal surface 304e of the knob body 304a and the interaction of the engagement features such as the threads 322 and 350 guide and releasably compress the slit end 324 of the shaft 306 to provide clamping of a fixation element, such as bone pin 600. In the case where no slits are provided to the end 324 of the shaft, or even if slits are provided, the end 324 of the shaft 306 can be tapered or have a funnel-like shape to match the tapered internal surface 304e of the knob body 304a. A portion of the shaft 306 or the stopper 318 can include an at least partially spherical surface to permit the shaft 306, and thus, the bone pin 600 or 700 disposed in the through-bore of the shaft 306 to orient relative to the clamp body 302, and can have at least one anti-rotation feature such as protrusion 320 adapted to sit in a key way 004 in the clamp body 302. Other anti-rotation features can be pins, recesses, splines, and the like. The shaft 306 is configured to extend through the clamp body 302 via the through-bores 000 in the upper and lower jaws 302a and 302b and into the through-bore of the knob 304 such that the stopper 318 is disposed in the clamp body 302 and at least a portion of the threads 322 of the shaft and the slit end 324 disposed inside the knob body 304a. The shaft threads 322 operably engage the internal threads 350 of the knob 304 in forming a threaded connection between the shaft 306 and the knob 304 to form a cannulation or reception for receiving a bone pin such as bone pin 600 of uniform diameter or bone pin 700 of varying diameter.

In operation, the tightening of the knob 304 shortens the distance between the knob 304 and the stopper 318 and thus, flexes the upper and lower jaws 302a and 302b towards each other to clamp on an external fixation element such as the first or second external fixation components 102 and 104 disposed in aperture 308. Simultaneously, the slit end 324 of the shaft 306 is pushed and guided by the tapered internal surface 304e of the knob body 304a toward the opposing end 304c of the knob 304 and compressed circumferentially onto the bone pin 600 or 700 at the opposing end 304c of the knob 304 as the slit end 324 is pushed through the smaller opening 002 at the opposing end 304c of the knob 304, and thus, clamping onto the bone pin 600 or 700 by interference fit.

The clamp body 302 can include an annular protrusion such as a convex annular protrusion 312 disposed adjacent to the through-bore of the upper jaw 302a for operably engaging with the clamp body facing end 304b of the knob 304 for secure engagement. The annular protrusion 312 can have engagement features on its external convex surface to lock angularly with other engagement features on an underside of the clamp body facing end 304b of the knob 304.

FIGS. 11-15 illustrate an alternative embodiment 400 of the closed-end clamp system 300. The open-end clamp device 400 is similar in design to the closed-end clamp device 300 except that the groove or aperture 408 is disposed adjacent to the open end 402c of the clamp body 402. The outer edges of the sides of the groove or aperture 408 along its length are chamfered to allow the clamp system 400 to easily snap onto a fixation element such as fixation components 102 and 104. The knob 404 has an under surface 428 having a rough surface such as a radial interdigitation pattern operably engaging a convex protrusion 412 having a rough surface such as circular steps disposed adjacent to the through-bore in the upper jaw 402a.

FIGS. 15A-15D illustrate an alternative embodiment 2600 of the open-end clamp system 400. The open-end

clamp system 2600 comprises a clamp body 2602, a knob 2604 and a shaft 2606. The clamp body 2602 having an open end 2602c and a close or hinged end 2602d connecting an upper jaw 2602a to a lower jaw 2602b forming a groove or aperture 2608 for receiving an external fixation element such as the first or second external fixation components 102 and 104, and a slot or spacing 2610 in communication with the aperture 2608. The upper and lower jaws 2602a and 2602b have through-bores 2000a and 2000b formed in at least partial alignment and dimensioned for receiving at least a portion of a locking element or assembly, such as the illustrated assembly comprising the knob 2604 and the shaft 2606. One of the through-bores 2000a and 2000b of the upper and lower jaws 2602a and 2602b, such as through-bore 2000b, defines a first diameter D1 and a second diameter D2, wherein D1 is smaller and located closer to the slot 2610. The inner surface 2602e containing D1 and D2 is shown as partially spherical, but it can be conical, partially conical or frusto-conical, or faceted. The inner surface 2602e is configured and dimensioned to operatively interact with an external surface of a slit portion of the shaft 2606 to clamp onto a fixation element, such as bone pin 600 or 700, received in a through-bore formed along a length of the shaft 2606.

The knob 2604 comprises a longitudinally formed through-bore having an internal thread and dimensioned for receiving and operatively interacting with the shaft 2606. Other engagement features, such as tabs and fins, can be used in place of or in addition to the thread on the internal surface of the knob 2604. The opposing end 2604c of the knob body 2604 can include one or more slits, such as slits 426a as shown in FIG. 11A for accommodating a broader range of dimensional tolerances of the bone pin 600 or 700. The knob 2604 can have an external surface and/or shape for providing a secure grip surface and optionally a hexagonally shaped geometry that interfaces with a wrench.

The variable position shaft or shaft 2606 includes an elongated body with a through-bore extending longitudinally along its length and dimensioned for receiving a fixation element, such as a bone pin 600 or 700, a locking or engagement feature such as threads 2622 on the external surface of the shaft 2606, and a stopper or an enlarged structure, such as head 2618, formed with one or more slits 2624 extending longitudinally along at least a portion of the length of the shaft 2606, and operatively interacting with at least a portion of an inner surface of one of said upper and lower jaws, such as inner surface 2602e, for compressing the slit stopper 2618 to clamp onto the bone pin 600 or 700. The inner surface 2602e also, but not necessary, prevents the shaft 2606 from passing completely through the clamp body 2602, or through at least one of the jaws 2602a or 2602b which the stopper 2618 first comes in contact with, such as the jaw 2602b. Other features and designs on the inner surface of the clamp body 2602, or of any of its upper and lower jaws that operatively interact with at least a portion of the shaft 2606 to prevent the shaft 2606 from passing completely through are still within the spirit and scope of the present invention. The stopper 2618 has a partially spherical external shape and at least one anti-rotation feature, such as anti-rotation pin 2620 configured to mate with a feature, such as a key way, on an inner surface of the clamp body 2602. Other anti-rotation features can be splines, recesses, protrusions or the like. Other shapes including conical and faceted external shapes of the stopper are considered within the spirit and scope of the present invention. The through-bore of the shaft 2606 and the width of the slit 2624 are dimensioned to receive a fixation element, such as bone pin

600 or 700, with very little play between the shaft 2606 and the bone pin 600 in an uncompressed state and a tight fit between the shaft 2606 and the bone pin 600 or 700 in a compressed state. The shaft 2606 can comprise a tapered end. The engagement feature 2622 on the external surface of the shaft 2606 can have other forms such as fins and tabs for interacting with the corresponding engagement feature on the inner surface of the knob 2604 to form a mechanical connection for clamping the fixation components and elements. The shaft 2606 is configured to extend through the clamp body 2602 via the through-bores in the upper and lower jaws 2602a and 2602b and into the through-bore of the knob 2604 such that the stopper 2618 is disposed in the clamp body 2602 and at least a portion of the threads 2622 of the shaft is disposed and operatively interacts with the threads on the inner surface of the knob 2604a.

FIGS. 16-17 and 17A describe an alternate embodiment 500 of the open-end clamp system 400. The open-end clamp system 500 is of a modular type. The open-end clamp system 500 is similar to the open-end clamp system 400 except that the convex annular protrusion 512 being a two-piece insert made of a separate upper part 504 and a separate lower part 506, and each of the parts 504 and 506 being formed with two key ways matching the key ways on the inner surfaces of the through-bores in the upper and lower jaws 502a and 502b of the clamp body 502 for receiving the anti-rotation features 320, or 420. The open-end clamp system 500 further includes a separate clip or insert 508 disposed between the upper and lower jaws 502a and 502b of the clamp body 502 for modifying the space therein. The insert 508 including an upper jaw jacket 508a connected to a lower jaw jacket 508b to form an insert groove 518 for laterally receiving a fixation element such as fixation components 102 or 104. A through-bore is formed in each of said upper and lower jaw jackets 508a and 508b of the insert 508 and aligned with aligned through-bores formed in the upper and lower jaws 502a and 502b of the clamp body 502 for receiving the convex annular protrusion insert 512. The insert 508 includes a slot or spacing between said jaw jackets 508a and 508b and in communication with said insert groove 518 to allow the upper and lower jaws 502a and 502b of the clamp body 502 and the jaw jackets 508a and 508b of the insert 508 to flex during locking and unlocking of the clamp system 500. The insert 508 is configured to have an outer cross-sectional shape (FIG. 17A) being substantially the same as an inner cross-sectional shape of the clamp body 502 to allow the insert 508 to easily slide into the space between the upper and lower jaws 502a and 502b of the clamp body 502 and mate or attach to the inner surface of the clamp body 502. The insert groove 518 can include splines to help secure gripping onto the fixation element.

Although the foregoing exemplary embodiments describe clamping systems having upper and lower jaws joined together by a hinged or closed end, the clamping systems of various embodiments of the present invention can comprise two or pairs of two separate upper and lower jaws spaced apart via a flexible structure, such as a spring coil surrounding a fastener, such as shaft 306, extending through the through-bores in the upper and lower jaws of the clamp to form one or more grooves for receiving external fixation elements such as rods, bars, pins, and a slot between the upper and lower jaws to allow the jaws to flex during locking and unlocking.

FIGS. 18-20 show an exemplary embodiment of an elbow-spanning hinged external fixation system 200 using the external fixator system including the novel clamp devices of the present invention. The system 200 is coupled

to a human elbow 10 comprising a humerus 12, ulna 14, and radius 16. FIGS. 21-22 show exploded views of the hinge or articulator of the system 200.

Now referring to FIGS. 18-22, the elbow-spanning hinged external fixation system 200 comprising a first external fixation component 202, a second external fixation component 204, a fastener 206, a closed-end clamp system 300 and an open-end clamp system 400. The first external fixation component 202 can be adapted to attach to the humerus 12, the ulna 14 and/or the radius 16 by use of the closed-end clamp system 300 and/or open-end clamp system 400 and fixation elements such as bone pins. The second external fixation component 204 can be adapted to attach to the humerus 12, the ulna 14 and/or the radius 16 by use of the closed-end clamp system 300 and/or open-end clamp system 400.

The first external fixation component 202, second external fixation component 204, fastener 206, closed-end clamp system 300 and open-end clamp system 400 can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque and/or other forces that may be applied to the system 200, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made biocompatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form a first external fixation component, a second external fixation component, a fastener, a closed-end clamp system and an open-end clamp system of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

In the illustrated embodiment 200 in FIGS. 18-22, the first external fixation component 202 comprises a first component proximal (e.g., first) end 208 having a straight portion with circular cross-sectional shape (FIG. 21A) and a first component distal (e.g., second) end 210 comprising a curved portion with a semi-circular cross-sectional shape (FIG. 21B) formed with a first pivot structure 222 having a circular cross-sectional shape (FIG. 22A), and a through-bore with an internal thread 232 and a rough end surface 224. The first component proximal end 208 can be straight or curved. The second external fixation component 204 comprises a straight portion of cylindrical structure and a curved portion with semi-circular cross-sectional shape (FIG. 21B), a second component distal (e.g., first) end 214 and a second component proximal (e.g., second) end 212 comprising the curved portion formed with a second pivot structure 226 having a circular cross-sectional shape (FIG. 22A), a through-bore with no internal threads and a rough end surface 228. The second component distal end 214 can be straight or curved. Each of the first and second external fixation components 202 and 204 including their respective pivot structures 222 and 226 can be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy). A fastener 206 having threads on its shaft 220 is configured to extend



through the through-bore in the cylindrical pivot structure **226** of the second external fixation component **204** and the through-bore in the cylindrical pivot structure **222** of the first external fixation component **202**, and forms a threaded connection with the cylindrical pivot structure **222**. The first external fixation component **202** and second external fixation component **204** are attached to each other via the fastener **206** to form a movable hinge or joint **230**. This movable hinge or joint **230** is then fixed in position by further tightening the fastener **206** which then interlocks the rough end surface **224** of the first pivot structure **222** with the rough end surface **228** of the second pivot structure **226**. Thus, the first external fixation component **202** and the second fixation component **204** are now locked in position to reduce the bone fracture. The fastener **206** can have a distal end **216** with irregularly shaped external geometry **218** to provide a secure gripping surface, and a shaft **220** with engagement features that can interface with the engagement features such as fins or threads **232** in the second external fixation component **204**.

The elbow-spanning hinged external fixation system **200** uses a combination of foregoing described embodiments of novel clamp systems **300**, **400**, and **500** for coupling the external fixation system **200** to the bone for fixing bone injury. This novel hinged system **200** significantly reduces surgical time by providing surgeons with flexibility in using the system on either side of the joint/body without having to align the mechanical pivot axis with the natural pivot axis of the joint, and ease of locking multiple fixation elements at once with a single tightening of a knob.

Referring now to FIGS. **23-25**, a first embodiment of an exemplary knee-spanning external fixation system **800** is illustrated mounted on a lower extremity **18** comprising a femur **20**, tibia **22**, fibula **24** and a foot **26**.

FIGS. **23-27** illustrate a first embodiment of an exemplary knee-spanning external fixation system **800** comprising a first external fixation component **802**, a second external fixation component **804**, a first fastener **806**, a second fastener **808**, a closed-end clamp system **300** and an open-end clamp system **400**. The first external fixation component **802** can be adapted to couple to the femur **20**, the tibia **22**, the fibula **24** and/or the foot **26** by use of the closed-end clamp system **300** and/or open-end clamp system **400**. The second external fixation component **804** can be adapted to attach to the femur **20**, the tibia **22**, the fibula **24** and/or the foot **26** by use of the closed-end clamp system **300** and/or open-end clamp system **400**.

The first external fixation component **802**, second external fixation component **804**, first fastener **806**, second fastener **808**, closed-end clamp system **300** and open-end clamp system **400** can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque and/or other forces that may be applied to the system **800**, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made biocompatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form a first external fixation component, a second external fixation component, a fastener, a closed-end clamp system and an open-end clamp

system of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

In the illustrated embodiment **800** in FIGS. **23-27**, the first external fixation component **802** comprises a straight portion of cylindrical structure and a curved portion also of cylindrical structure, a first component proximal (e.g., first) end **810** and a first component distal (e.g., second) end **812** comprising the curved portion formed with a pivot structure of cylindrical body **814** having a through-bore bound by smooth walls extending along its pivot axis and further having a rough end surface **834**. The first component proximal end **810** can be straight or curved. The second external fixation component **804** comprises a straight portion of cylindrical structure and a curved portion also of cylindrical structure, a second component distal (e.g., first) end **818** and a second component proximal (e.g., second) end **816** comprising the curved portion formed with a pivot structure of cylindrical body **820** having a through-bore bound by smooth walls extending along its pivot axis and a rough end surface **836**. The second component distal end **818** can be straight or curved. The pivot structures **814** and **820** each has a length along the pivot axis such that when the two pivot structures **814** and **820** are joined end to end at their rough surfaces by a fastener, such as **806** or **808**, the first external fixation component **802** and the second external fixation component **804** are disposed on different sides of the bone or knee (e.g., right side, left side, anterior, posterior). Each of the first and second external fixation components **802** and **804** including their respective pivot structures **814** and **820** can be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy). A fastener **806** having threads **826** on its shaft is configured to extend through the through-bore in the cylindrical pivot structure **814** of the first external fixation component **802** and the through-bore in the cylindrical pivot structure **820** of the second external fixation component **804** and into a second fastener such as a threaded nut **808**, and forms a threaded connection with the nut **808**. The first external fixation component **802** and second external fixation component **804** are thus attached to each other via the coupling and interactions of the pivot structures **814** and **820** and the fasteners **806** and **808** to form a movable hinge or joint **838**. This movable hinge or joint **838** is then locked in position by further tightening the fasteners **806** and **808** which interlocks the rough end surface **834** of the first external fixation component **802** with the rough end surface **836** of the second external fixation component **804**. The fastener **806** can have a distal end or head **822** with irregularly shaped external geometry **824** to provide a secure gripping surface, and a shaft with engagement features such as threads **826** that can interface with the engagement features such as fins or threads inside the second fastener **808**. Similarly, the second fastener **808** can also have an outer surface geometry for secure gripping surface.

FIGS. **28-32** illustrate an alternative embodiment **900** of the exemplary knee-spanning external fixation system **800** comprising a first external fixation component **902**, a second external fixation component **904**, a first fastener **906**, a second fastener **908** and an open-end clamp system **400**. The first external fixation component **902** can be adapted to attach to the femur **20**, the tibia **22**, the fibula **24** and/or the foot **26** by use of the closed-end clamp system **300** and/or

open-end clamp system **400**. The second external fixation component **904** can be adapted to attach to the femur **20**, the tibia **22**, the fibula **24** and/or the foot **26** by use of a closed-end clamp system **300** and/or open-end clamp system **400**.

The exemplary knee-spanning external fixation system **900** is similar to the foregoing described system **800** except that the lockable and movable hinge of the knee-spanning external fixation system **900** is dimensioned to accommodate a wider joint or bone size. This is made possible by designing the pivot structures **914** and **920** to have a longer length along their mechanical pivot axis for accommodating a broader range of pin sites and/or body or joint sizes.

FIGS. **33-37** show a third embodiment of an exemplary knee-spanning external fixation system **1000** for mounting on a lower extremity **18** comprising a femur **20**, tibia **22**, fibula **24** and a foot **26**.

The third embodiment of an exemplary knee-spanning external fixation system **1000** comprises a first external fixation component **1002**, a second external fixation component **1004**, a first fastener **1006**, a second fastener **1008** and an open-end clamp system **400** or a close-end clamp system **300**. The first external fixation component **1002** can be adapted to couple to the femur **20**, the tibia **22**, the fibula **24** and/or the foot **26** by use of the closed-end clamp system **300** and/or open-end clamp system **400**. The second external fixation component **1004** can be adapted to couple to the femur **20**, the tibia **22**, the fibula **24** and/or the foot **26** by use of a closed-end clamp system **300** and/or open-end clamp system **400**.

The first external fixation component **1002**, second external fixation component **1004**, first fastener **1006**, second fastener **1008** and open-end clamp system **400** and optionally close-end clamp system **300** can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque and/or other forces that may be applied to the system **1000**, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made biocompatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form a first external fixation component, a second external fixation component, a fastener, a closed-end clamp system and an open-end clamp system of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

In the illustrated embodiment **1000** in FIGS. **33-37**, the first external fixation component **1002** having an "L" shape and a circular cross-sectional shape, comprises a first component proximal (e.g., first) end portion **1010** and a first component distal (e.g., second) end portion **1012**. The first component distal end portion **1012** comprises the shorter leg of the "L" shape and is coupled to or formed at its open end a pivot structure of cylindrical body **1014** having a through-bore bound by smooth walls extending along its pivot axis and a rough end surface **1034**. The first component distal end portion **1012** comprises a straight middle segment connecting two curved end segments. However, these segments can all be straight or curved. The first component proximal end

**1010** can be straight or curved. The second external fixation component **1004** having an inverted "L" shape, comprises a second component proximal (e.g., second) end portion **1016** and a second component distal (e.g., second) end portion **1018**. The second component proximal end portion **1016** comprises the shorter leg of the inverted "L" shape and is coupled to, or formed at, its open end a pivot structure of cylindrical body **1020** having a through-bore bound by smooth walls extending along its pivot axis and a rough end surface **1036**. The second component proximal end portion **1016** comprises a straight middle segment connecting two curved end segments. However, these segments can all be straight or curved. The second component distal end portion **1018** can be straight or curved. The pivot structures **1014** and **1020** each has a length along the pivot axis such that when the two pivot structures **1014** and **1020** are joined end to end at their rough surfaces **1034** and **1036** by a fastener, the first external fixation component **1002** and the second external fixation component **1004** are disposed on different sides of the bone or knee (e.g., right side, left side, anterior, posterior). Each of the first and second external fixation components **1002** and **1004** including their respective pivot structures **1014** and **1020** can be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy).

A fastener **1006** having threads **1026** on its shaft is configured to extend through the through-bore in the cylindrical pivot structure **1014** of the first external fixation component **1002** and the through-bore in the cylindrical pivot structure **1020** of the second external fixation component **1004** and into a second fastener such as a threaded nut **1008**, and forms a threaded connection with the nut **1008**. The first external fixation component **1002** and second external fixation component **1004** are thus attached to each other via fasteners **1006** and **1008** to form a movable hinge or joint **1038**. This movable hinge or joint **1038** is then locked in position by further tightening the fasteners **1006** and **1008** which interlocks the rough end surface **1034** of the pivot structure **1014** with the rough end surface **1036** of the pivot structure **1020**. The fastener **1006** can have a distal end or head **1022** with irregularly shaped external geometry **1024** to provide a secure gripping surface, and a shaft with engagement features such as threads **1026** that can interface with the engagement features such as fins or threads inside the second fastener **1008**. Similarly, the second fastener **1008** can also have an outer surface geometry for secure gripping surface.

In this exemplary embodiment, the first component distal end portion **1012** and the second component proximal end portion **1016** form a right angle with their respective first component proximal end portion **1010** and second component distal end portion **1018**. One skilled in the art can select other angles such as 60 or 120 degrees to accommodate the type of fracture or body shape, for example. Other shapes and dimensions of the first and second external fixation components **1002** and **1004** also are within the spirit and scope of various embodiments of the present invention. Similarly, the angles ( $\theta_1$ ,  $\theta_2$ ) between the pivot structures **1014** and **1020** and their respective first component distal end portion **1012** and second component proximal end portion **1016** are 90 degrees as schematically illustrated in FIGS. **33-37**, but angles other than 90 degrees are contem-

plated and within the spirit and scope of various embodiments of the present invention.

The first external fixation component **1002** and the second external fixation component **1004** including their respective pivot structures **1014** and **1020** can each be formed as a unitary modular structure or a modular structure. In the case of a unitary modular structure, for example, the first external fixation component **1002** can be formed from a single rod or bar and bent into the “L” shape, and welded to the pivot structure **1014**. In the case of a modular structure, the first external fixation component **1002** and the pivot structure **1014** can be formed by removably connecting plurality of straight and/or curved rod segments and the pivot structure **1014** by snap-fitting, or threading, for example. The first and second external fixation components **1002** and **1004** and the pivot structures **1014** and **1020** can have any cross-sectional shapes (e.g. hexagonal, oval, square) and dimensions other than the circular cross-sectional shape as schematically illustrated in FIGS. **33-37**.

Referring now to FIGS. **38-39**, an alternative embodiment **1100** of the exemplary knee-spanning external fixation system **1000** is shown mounted by pins on the lower extremity **18** comprising a femur **20**, tibia **22**, fibula **24** and a foot **26**.

The knee-spanning external fixation system **1100** illustrated in FIGS. **38-41** is similar to exemplary knee-spanning external fixation system **1000** in FIGS. **33-37** except that the first component distal (e.g., first) end **1112** and the second component proximal (e.g., second) end **1116** are each connected to their respective pivot structures **1114** and **1120** at an angle greater than 90 degrees ( $\theta_3$ ,  $\theta_4$ ).

FIGS. **42-69** show various exemplary ankle-spanning external fixation systems, some are of unitary, prefabricated modular construction (e.g. from multiple pieces welded together), or unitary construction (e.g. from a single piece of material by molding), while others are of modular construction (e.g. multiple pieces removably threaded together to allow surgeons to use the assembled system as is or to reconfigure the assembled system to match the patient anatomy). The illustrated ankle-spanning external fixation systems comprise a proximal or upper frame coupled to a distal or lower frame such as the curved foot frame including a posterior frame segment extending angularly from and above an inferior frame segment designed for placement and use substantially adjacent to the ankle area of the body to protect both the posterior and the inferior of a foot or ankle while healing is taken place. The system can be used adjacent to other joints such as the elbow or the knee, and is capable of being any shape and size that allows for support of the joint and area round the joint such as the foot, ankle, and/or lower extremity.

Referring now to FIGS. **42-44**, a first embodiment of an exemplary ankle-spanning external fixation system **1200** is shown mounted via pins on an exemplary lower extremity **28** comprising a tibia **32**, fibula **34** and a foot **36**. The fixation system **1200** includes one or more open-end clamps **400** and **1300** and optionally closed-end clamps for clamping fixation elements such as bars, rods, pins, or wires of various diameters.

The external fixation system **1200** and open-end clamp systems **400** and **1300** can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque and/or other forces that may be applied to the system **1200**, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made bio-

compatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form the system **1200** of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

The illustrated embodiment **1200** in FIGS. **42-44** comprises two ankle-spanning external fixation systems **1200** which are substantially the same and mounted on each side of the foot to protect the ankle and area around the ankle. Each external fixation system **1200** comprises a single piece, unitary prefabricated modular frame comprising a proximal (e.g., first) frame **1200a**, a connector **1214** and **1216** and a distal (e.g., second) frame **1212** attached together by standard means, such as welding, soldering, brazing, crimping, or adhesives. The proximal frame defines a single bar or rod such as bar **1200a** including a proximal (e.g., first) end portion **1202** and a distal (e.g., second) end portion **1204** and a curved portion **1206** connecting the proximal and distal end portions **1202** and **1204**. The distal end **1204** can be of a reduced diameter **1208** and comprises an extension or outrigger **1210** which can be divided into two or more branches, such as bifurcation **1220**, for attaching a clamp such as the open-end clamp system **300** or closed-end clamp system **400**. A distal frame, such as the foot frame **1212**, configured to capture the posterior and the inferior aspects of a joint, such as the ankle, comprising two parallel curved rods **1218**, is coupled to the proximal frame, such as the bar **1200a**, via a Y-shaped connector having two arms **1216** and a trunk **1214**. Other shapes of the connector also are within the spirit and scope of various embodiments of the present invention. Each curved rod **1218** comprises a straight inferior (e.g., first) frame section or portion **1218a** and a straight posterior (e.g., second) frame section or portion **1218b** and a curved frame section or portion **1218c** connecting the straight inferior frame section **1218a** to the straight posterior frame section **1218b**, wherein said inferior frame portion **1218a** and said posterior frame portion **1218b** are operatively disposed in at least partially surrounding and spatial relation to the ankle or the heel of the foot **36**, wherein said posterior frame portion **1218b** extends angularly from and above said inferior frame portion **1218a**. Each arm **1216** of the Y-shaped connector connects to one of the rods **1218** of the foot frame **1212** at the concave surface side of the curved frame section, and the trunk **1214** of the Y-shaped connector connects to the curved portion **1206** of the proximal frame such as the bar frame **1200a** at the convex surface side of the curved portion **1206**.

The foot frame **1212** is generally configured to capture the posterior and the inferior aspects of a foot or ankle and thus may take various shapes as illustrated in other exemplary embodiments. In the single piece, unitary modular construction, the proximal and distal frames **1200a** and **1212** and connector(s) **1214** and **1216** and their subcomponents such as outrigger **1220** can be welded, soldered, crimped, brazed or glued/epoxied together during manufacturing. Alternatively, in a unitary construction, the proximal frame **1200a**, the connector **1214** and **1216** and the distal frame **1212** and optionally any subcomponents such as an outrigger **1220** may be integral-machined or formed from a single piece of metal or other material by standard means such as molding or machining. In a multi-piece, or modular construction, the proximal and distal frames **1200a** and **1212** and connector

1214 and 1216 and their subcomponents 1220 can be removably connected by standard means such as threads, plug-socket joint, snap-fit, interference fit or a combination thereof during manufacturing or immediately prior to use to provide surgeons the flexibility of design choices to fit the patient anatomy. The proximal and distal end portions 1202 and 1204 of the bar frame 1200a and the Y-shaped connector may be formed of various curved and/or straight pieces or subcomponents connected together and may have any profiles. The components of the system 1200 are shown as having circular cross-sectional shape. Other cross-sectional shapes such as hexagonal shape, square, rectangle, for example, are within the spirit and scope of the various embodiments of the present invention.

Referring now to FIGS. 45-47, an alternative embodiment 1400 of the exemplary ankle-spanning external fixation system 1200 is shown mounted by pins on the lower extremity 28 comprising a femur 30, tibia 32, fibula 34 and a foot 36, wherein the foot frame is of a different design.

The exemplary ankle-spanning external fixation system 1400 comprises a single piece, unitary prefabricated modular frame comprising a proximal (e.g., first) frame 1400a, a connector 1414 and a distal (e.g., second) frame 1412 attached together by standard means such as welding, soldering, brazing, crimping, or adhesives. Alternatively, the proximal frame, the connector and the distal frame may be integral-machined or formed from a single piece of metal or other material by standard means such as molding or machining. The exemplary ankle-spanning external fixation system 1400 comprises a proximal frame such as bar frame 1400a coupled to a distal frame such as a foot frame 1412 via a frame connector 1414 wherein the foot frame comprises a continuous elongated ring frame having a U-shaped inferior (e.g., first) frame section 1418 lying in a first plane and a U-shaped posterior (e.g., second) frame section 1416 lying in a second plane and a curved section 1420 connecting each of the legs of the U-shape inferior frame section 1418 to each of those of the U-shaped posterior frame section 1416 to form a closed loop. Other shapes of the inferior and posterior frame portions are also within the spirit and scope of various embodiments of the present invention. The first and second planes containing the inferior frame section 1418 and the posterior frame section 1416 are perpendicular to each other as schematically illustrated. However, the angle between the first and second planes can be other than 90 degrees, such as 60 degrees or 120 degrees. Said inferior frame portion 1418 and said posterior frame portion 1416 are operatively disposed in at least partially surrounding and spatial relation to the ankle or the heel of the foot 36, wherein said posterior frame portion 1416 extends angularly from and above said inferior frame portion 1418. In the single piece, unitary modular construction, the proximal and distal frames 1400a and 1412 and connector(s) 1414 and their subcomponents such as outrigger 1410 can be welded, soldered, crimped, brazed or glued/epoxied together during manufacturing. Alternatively, in a unitary construction, the proximal frame 1400a, the connector 1414 and the distal frame 1412 and optionally any subcomponents such as an outrigger 1410 may be integral-machined or formed from a single piece of metal or other material by standard means such as molding or machining. In a multi-piece, or modular construction, the proximal and distal frames 1400a and 1412 and connector 1414 and their subcomponents 1410 can be removably connected by standard means, such as threads, plug-socket joint, snap-fit, interference fit or a combination thereof during manufacturing or immediately prior to use to provide surgeons the

flexibility of design choices to fit the patient anatomy. All the components of the frames and the frame connector can have circular cross-sectional shape as shown or can have other cross-sectional shape including square, oval, hexagon, or others. Each of the proximal and distal frames can be made from a single rod/bar or a plurality of straight and/or curved bar/rod segments or subcomponents connected together end-to-end using welding, soldering, gluing, brazing, crimping, threading, snap-fitting or the like.

Referring now to FIGS. 48-50, a third embodiment of an exemplary ankle-spanning external fixation system 1500 is illustrated mounted on a lower extremity 28 comprising a tibia 32, fibula 34 and a foot 36.

FIGS. 48-52 illustrate a third embodiment of an exemplary ankle-spanning external fixation system 1500 comprises a proximal frame including a first external fixation component 1502a, a second external fixation component 1502b, and a fastener 1506, and connecting to a distal (e.g., first) frame such as foot frame 1504, and open-end clamp systems 400 and 1300. The ankle-spanning external fixation system 1500 can be adapted to couple to the tibia 32, the fibula 34 and/or the foot 36 by use of a closed-end clamp system 300 and/or the open-end clamp systems 400 and 1300.

The first and second external fixation components 1502a and 1502b, and the foot frame 1504, fastener 1506 and open-end clamp systems 400 and 1300 can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque and/or other forces that may be applied to the system 1500, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made biocompatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form the first external fixation component, the second external fixation component, the foot frame, the fastener, and the open-end clamp systems of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

In the illustrated embodiment 1500 in FIGS. 48-52, a proximal (e.g., second) bar frame comprises a first external fixation component 1502a comprising a straight first component proximal (e.g., first) end portion 1508 and a curved first component distal (e.g., second) end portion 1510 including a first pivot structure 1512a comprising a rough surface 1514a and a threaded shaft centered and formed perpendicularly on the rough surface 1514a, and said first external fixation component 1502a pivotally coupled and locked to a second external fixation component 1502b comprising a straight second component proximal (e.g., first) end portion 1534, a straight second component distal (e.g., second) end portion 1518 of a reduced diameter, and a curved or arc portion 1532 connecting the second component proximal end portion 1534 and a second component distal end portion 1518, said arc portion 1532 having a pivot structure 1512b with a rough surface 1514b and a centered through-bore for receiving the threaded shaft of the pivot structure 1512a to form a movable joint or hinge. A fastener, such as threaded nut 1506, is coupled to the threaded shaft

of the first pivot structure **1512a** to form a threaded connection to lock the movable joint, thus, also locking the first and second external fixation component **1502a** and **1502b** in place. The interaction between the rough surfaces **1514a** and **1514b** in a locking state provides anti-rotation to the first and second fixation components **1502a** and **1502b**. The second component proximal end portion **1534** is attached by, for example, welding, soldering or gluing to a distal frame, such as the foot frame **1504**, to form a unitary, prefabricated modular structure. Alternatively, the foot frame **1504** can be integrally machined or formed with the second external fixation component **1502b** from a single piece of metal or other material to form a unitary structure. The foot frame **1504** comprises a straight posterior segment **1516a**, a straight inferior segment **1516b**, and a curved or arc segment **1516c** connecting the straight posterior segment **1516a** and the straight inferior segment **1516b** to form a curved frame or rod or bar for protecting and supporting both the posterior and the inferior aspects of a foot or joint such as the ankle while healing is taken place. Said inferior frame portion **1516b** and said posterior frame portion **1516a** are operatively disposed in at least partially surrounding and spatial relation to the ankle or the heel of the foot **36**, wherein said posterior frame portion **1516a** extends angularly from and above said inferior frame portion **1516b**. The second component distal end portion **1518** has a smaller diameter and is attached (e.g. welded, soldered or glued) to an outrigger **1522** used as a clamp attachment, for example. The outrigger **1522** can also be integrally machined or formed with the second external fixation component **1502b**.

The first and second component proximal end portions **1508** and **1534**, the first and second component distal end portions **1510** and **1518**, and more generally the first and second external fixation components **1502a** and **1502b** and the posterior and inferior segments **1516a** and **1516b** can be straight or curved. The first and second external fixation components **1502a** and **1502b** and the foot frame **1504** of the system **1500** can have any cross-sectional shapes such as circle, square, rectangle, hexagon, etc., and can have uniform diameter or varied diameter along their lengths. The first and second external fixation components **1502a** and **1502b** including the foot frame **1504** of the system **1500** can each be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy).

The pivot structures **1512a** and **1512b** can have any cross-sectional shapes, not just limited to a circular shape as illustrated in this example. The pivot structures **1512a** and **1512b** can also have any lengths or thickness as measured along its pivot axis. The pivot structures **1512a** and **1512b** of the movable hinge or joint can each also be an integral part of (e.g. integrally formed with) or a separate part to (e.g. removably coupled to) their respective first external fixation component **1502a** and second external fixation component **1502b**. The rough surfaces **1514a** and **1514b** can include serration or radial interdigitation or combinations thereof. In a system where both pivot structures **1512a** and **1512b** each comprises a through-bore, a second fastener having a head and a threaded shaft can be used to couple the pivot structures **1512a** and **1512b** and operably interacts with the threaded nut **1506** to lock the pivot structures **1512a** and **1512b**. The fastener(s) can have a secure gripping surface for ease of handling during surgery. As illustrated, the first external fixation component **1502a** and the second external

fixation component **1502b** including the foot frame **1504** each is made as a unitary modular structure. In the modular structure, the first external fixation component **1502a** and the second external fixation component **1502b** and the foot frame **1504** can each be made from a plurality of straight and/or curved segments connected via threads, snap-fit or interference fit.

Referring now to FIGS. **53-57**, a fourth embodiment of an exemplary ankle-spanning external fixation system **1600** is shown mounted on an exemplary lower leg **28** comprising a tibia **32**, fibula **34** and a foot **36**.

FIGS. **53-61** illustrate a fourth embodiment of an exemplary ankle-spanning external fixation system **1600** comprising a proximal (e.g., first) frame having a first external fixation component **1602** and a second external fixation component **1604**, a proximal frame connector **1606**, and a distal (e.g., second) frame or a foot frame **1608**, a distal frame connector **1650**, a cartridge system **1610** and an open-end clamp system **400**. The ankle-spanning external fixation system **1600** can be adapted to attach to the tibia **32**, the fibula **34** and/or the foot **36** by use of a closed-end clamp system **300** and/or the open-end clamp systems **400** and **1300** and other fixation elements such as bone pins **600** or **700**.

The first external fixation component **1602**, the second external fixation component **1604**, the proximal (e.g., first) frame connector **1606**, the foot frame **1608**, the distal (e.g., second) frame connector **1650**, the cartridge system **1610** and the open-end clamp system **400** can be formed of any suitable material known to one skilled in the art that provides an adequate stiffness or resistance to torsion, stress, torque and/or other forces that may be applied to the system **1600**, including the structural arrangement at a fixation site and/or the material forming the components of an external fixation system. Example suitable materials include, but are not limited to, biocompatible materials, materials that can be made biocompatible, ceramics, polymers, polyethylene, ultra-high-molecular-weight polyethylene (UHMWPE), shape memory polymer, carbon fiber, metal, metal alloy, shape memory metals, tantalum, titanium (Ti), and cobalt alloys (e.g., cobalt-chromium (CoCr), cobalt-chromium-molybdenum (CoCrMo)). The material is also preferably, but not necessarily, radiolucent. It is considered advantageous to form the first external fixation component, the second external fixation component, the third external fixation component, the fourth external fixation component, the cartridge system and the open-end clamp system of aluminum, stainless steel and/or carbon fiber, at least because these materials have properties that are well suited to external fixation of fractures.

In the illustrated embodiment **1600** in FIGS. **53-61**, the proximal frame comprises the first external fixation component **1602** and the second external fixation component **1604**. The external fixation component **1602** comprises a first component proximal (e.g., first) end portion **1612** and a first component distal (e.g., second) end portion **1614** integrally formed with or coupled to a pivot structure **1616** having a rough surface **1618** and a through-bore bound by an inner surface having engagement features such as threads and key ways **1620** configured for receiving and connecting to at least a portion of the cartridge system **1610** for coupling to a bone and locking the system **1600**. The second external fixation component **1604** comprises a second component distal (e.g., first) end portion **1624** and a second component proximal (e.g., second) end portion **1622** integrally formed with or coupled to a pivot structure **1626** having a rough surface **1628** and a through-bore bound by an inner surface

having engagement features such as threads and key ways **1630** configured for receiving and connecting to at least a portion of the cartridge system **1610** for coupling to a bone and locking the external fixation components **1602** and **1604** in position.

The first and second external fixation components **1602** and **1604** can be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy). The first and second component proximal end portions **1612** and **1622** and the first and second component distal end portions **1614** and **1624** can be straight or curved. The first and second external fixation components **1602** and **1604** can have any cross-sectional shapes such as circle, oval, triangle, rectangle, square, polygonal shape. The first and second external fixation components **1602** and **1604** can have any uniform or varied diameter or thickness along their lengths. The pivot structures **1616** and **1626** can have any external cross-sectional shapes, not limited to just circular shape as illustrated in this example. The pivot structures **1616** and **1626** can also have any lengths or thickness as measured along its pivot axis. The pivot structures **1616** and **1626** can also be integrally formed with or removably coupled to their respective first external fixation component **1602** and second external fixation component **1604**. The rough surfaces **1618** and **1628** can include serration or radial interdigitation or combinations thereof.

The proximal frame connector **1606** comprises an elongated body comprising a connector proximal end portion **1634** integrally formed with or coupled to a pivot structure **1636** having a rough surface **1638** and an opposing rough surface **1640** and a through-bore connecting the two opposing surfaces **1638** and **1640** bound by an inner surface configured (e.g. key ways **1642**) for receiving and locking onto at least a portion of the cartridge system **1610**, and a bifurcated connector distal end portion including a pair of movable portions **1644** that are movable to flex toward and away from each other and arranged with one or more protrusions **1648** to engage with a hole **1654** in a distal frame connector **1650** of the lower frame such as the foot frame **1608**.

The distal frame such as the foot frame **1608** comprises a ring frame configured to protect both the posterior and inferior aspects of a foot or the ankle. The ring frame comprises a multiple curved elongated body structure defining a first curved side rod spaced apart and parallel to a second curved side rod wherein a first end connector extending from said first curved side rod to said second curved side rod in said inferior portion and a second end connector extending from said first curved side rod to said second curved side rod in said posterior portion. Said inferior frame portion and said posterior frame portion are operatively disposed in at least partially surrounding and spatial relation to the ankle or the heel of the foot **36**, wherein said posterior frame portion extends angularly from and above said inferior frame portion. The foot frame **1608** has a curvature from inferior to posterior with its concave surface orienting toward the heel of the foot. The foot frame **1608** further comprises a distal frame connector **1650** with a through-bore extending longitudinally through at least a portion of the elongated body **1650** for receiving the bifurcated connector distal end portion **1644**, and one or more holes **1654** for engaging with the one or more protrusions **1648** on the bifurcated connector distal end portion **1644**. The elongated

body **1650** is attached to a portion of one of the first and second curve side rods. The arrangement of the multiple holes **1654** along the distal frame connector **1650** provides adjustability to the spatial relation between the foot frame **1608** and the heel or the ankle. The foot frame including the distal frame connector and the proximal frame connector can be formed as a unitary, prefabricated modular component (e.g. from multiple pieces welded together), a unitary component (e.g. from a single piece of material by molding), or a modular component (e.g. multiple pieces removably threaded together to allow surgeons to use as-is or to reconfigure to match the patient anatomy).

The cartridge system **1610** for coupling the system to a bone portion via a bone pin **600** or **700** and locking the pivot structures **1616**, **1626**, and **1636**, and thus, also locking the ankle-spanning external fixation system **1600** comprises a knob **1658**, a main body **1660**, a variable position shaft **1662** and a retaining clip **1664**.

The knob **1658** comprises a knob body **1658a** having a main body facing end **1658b** and an opposing end **1658c**. The knob body **1658a** includes a funnel-like or frusto-conical internal surface or an internal surface having one or more tapered facets to receive and alternatively circumferentially compress and release a slit end or a funnel-like or tapered external surface of the shaft **1662** for clamping a fixation element such as bone pin **600**. The funnel-like or frusto-conical internal surface or more generally the through-bore bound by walls extending from the main body facing end **1658b** to the opposing end **1658c** of the knob body **1658a** is designed to be larger toward the main body facing end **1658b** than toward the opposing end **1658c** of the knob body **1658a**, and includes a first locking feature such as threads **1658d**. The tapered or conical internal surface inside the knob body **1658a** can be replaced with a taper insert. The opposing end **1658c** of the knob body **1658a** can include one or more slits or breakable lines for accommodating a broader range of dimensional tolerances of the bone pin **600** or **700**. The knob **1658** can have irregularly shaped geometry **1666** for providing a secure grip surface and optionally a hexagonally shaped geometry **1668** that interfaces with a wrench.

The variable position shaft or shaft **1662** includes an end portion including a stopper or an enlarged structure or structures such as a head **0016** for preventing the shaft **1662** from passing completely through the main body **1660**, and a locking or engagement feature such as threads **1678** on the external surface of the shaft **1662**, and one or more breakable lines or slits **1672** on an opposing end portion of the shaft. The slit end **1672** of the shaft **1662** can be tapered to match the tapered internal surface of the knob body **1658a**. The funnel like or tapered internal surface of the knob body **1658a** preferably interacts via the engagement features, such as the threads **1658d** and **1678**, with the externally tapered or funnel-like surface or the slit end **1672** of the shaft **1662** to provide clamping. The through-bore or opening in the opposing end **1658c** of the knob **1658** has a diameter smaller than the uncompressed diameter of the slit end **1672** of the shaft **1662** to provide interference fit among the inner surface of the knob **1658**, the slit end **1672** and the bone pin such as bone pin **600** or **700**. The shaft **1662** is configured to extend through the main body **1660** and into the through-bore of the knob **1658** such that the stopper **0016** is disposed in the main body **1660** and at least a portion of the threads **1678** of the shaft **1662** and the slit end **1672** disposed outside the main body **1660** and inside the knob body **1658a**. The shaft threads **1678** operably engage the internal threads **1658d** of the knob **1658** in forming a threaded connection

with the knob **1658** to form a cannulation or reception for receiving a bone pin, such as bone pin **600**, of uniform diameter, or bone pin **700** of varying diameter. A portion of the shaft **1662** or the stopper **0016** can include an at least partially spherical surface to permit the bone pin **600** or **700** to orient relative to the main body **1660**, and can have at least one anti-rotation feature such as protrusion **1676** adapted to sit in a key way in the main body **1660**.

In operation, the tightening of the knob **1658** pushes the slit end **1672** of the shaft **1662**, guided by the tapered internal surface or structure of the knob body **1658a**, toward or through the opposing end **1658c** of the knob **1658**. The slit end **1672** is compressed circumferentially onto the bone pin **600** or **700** at the opposing end **1658c** of the knob **1658** as the slit end **1672** is pushed through the smaller opening at the opposing end **1658c** of the knob **1658**, and thus, clamping onto the bone pin **600** or **700** by interference fit.

The main body **1660** is configured to extend through the pivot structures **1616**, **1626**, and **1636** of the first and second external fixation components **1602** and **1604** and the connector **1606**. The main body **1660** has a cylindrical body with proximal protrusions **1682** for engaging with key ways **1620** on the inner surface of the pivot structure **1616** of the first external fixation component **1602** and distal protrusions **1684** for engaging with key ways **1630** on the inner surface of the pivot structure **1626** of the second external fixation component **1604**. The main body **1660** has inner surface configured to operably interact with the shaft **1662** to provide both angular rotation of the shaft **1662** relative to the main body **1660** and anti-rotation of the shaft **1662** during locking. The inner surface of the main body includes one or more key way **1686** for capturing the protrusions **1676** of the shaft **1662** for rotational stability, concave surfaces **1688** for interacting with the at least partially spherical stopper **0016** of the shaft **1662** and tapered or conical surface **1690** for providing angular rotation of the shaft **1662**, and slotted geometry **1692** that accepts a ring clip **1664** for preventing the variable position shaft **1662** to exit the main body **1660** once the cartridge system **1610** is completely assembled.

The ankle-spanning external fixation system **1600** is assembled by firstly, snap-fitting together the first external fixation component **1602**, the second external fixation component **1604** and the connector **1606** via male/female ends on their pivot structures **1616**, **1626** and **1636**. When the first external fixation component **1602**, the second external fixation component **1604** and the connector **1606** are rotated into their closed state, the key ways **1620**, **1630** and **1642** of the respective pivot structures **1616**, **1626** and **1636** become aligned and allow the assembled cartridge system **1610** to slide in. Once the cartridge system **1610** is in place, the first external fixation component **1602**, the second external fixation component **1604** and the connector **1606** can be opened up to the desired position according to anatomical considerations. Once the current embodiment **1600** is deployed and in position, the cartridge system can be adjusted and then locked in place by further tightening knob **1658**, which in turn locks the first external fixation component **1602**, the second external fixation component **1604** and the connector **1606** via the interactions of rough surfaces **1618**, **1638**, **1640** and **1628**.

Referring now to FIGS. **62-64**, an alternative embodiment **1700** of the ankle-spanning external fixation system **1600** is illustrated wherein the system **1700** includes the curved foot frame **1706** comprising a U-shaped posterior (e.g., first) frame section and a U-shaped inferior (e.g., second) section connected at the base by a straight frame section. The two U-shaped frame sections are arranged to lie on different

planes forming an angle of about 90 degrees. Other angles also lie within the spirit and scope of the various embodiments of the present invention.

Referring now to FIGS. **65-69**, an alternative embodiment **1800** of the ankle-spanning external fixation system **1700** is illustrated wherein the first external fixation component **1802**, second external fixation component **1804**, and the foot frame **1810** are each of modular construction, comprising two or more straight and/or curved segments joined together via plug-socket joints and fixed in place by threading, snap-fitting or interference-fitting. Each of the first external fixation component **1802**, second external fixation component **1804**, and the foot frame **1810** of the system **1800** can also be made into a unitary structure or unitary modular structure by molding or forming permanent connection among the subcomponents or segments by welding, soldering, crimping, brazing, and gluing/epoxying. The system **1800** can be single-use or disposable.

Referring now to FIG. **70**, a flow diagram of an embodiment of a method **3000** for fixating a bone fixator system about a target joint is shown. The method may be performed by a variety of users, including healthcare professionals, technicians, and patients installing and/or adjusting the bone fixator system. The bone fixator system used to implement the method may be or include features of any of the fixation systems disclosed herein (e.g., external fixation systems **100**, **200**, **800**, **900**, **1000**, **1100**, **1200**, **1400**, **1500**, **1600**, **1700**, **1800**, etc.) and the clamping devices used herein to implement the method may be or include features of any of the clamping devices and systems disclosed herein (e.g., clamp systems **300**, **400**, **500**, **1300**, **2600**, etc.).

At **3010**, components of a bone fixator system are aligned with target bone(s) about a target joint to be fixated. The target joint may be an elbow, a knee, an ankle, etc. For example, the bone fixator system may include a first fixation component and a second fixation component, the first fixation component may be aligned relative to a first target bone disposed adjacent to the target joint, and the second fixation component may be aligned relative to a second target bone disposed adjacent to the target joint on another side of the knee from the first target bone.

A clamp is also aligned relative to a target bone. For example, a clamp may be aligned with the target bone based on a desired position and/or orientation of a bone pin to be attached to the bone and secured or otherwise received by the clamp. The clamp may also be received on one of the fixation components of the bone fixator system while aligning the clamp.

At **3012**, a bone pin is attached (e.g., secured, coupled, drilled in, etc.) to a target bone using a clamp as a drill guide. For example, the clamp may define a through-bore configured to receive the bone pin. The through-bore may be used to sight or otherwise identify a target position on a surface of the target bone at which the bone pin is to be attached to the target bone. The bone pin is received through the through-bore of the clamp, and may be drilled into the bone. The clamp may be locked about the bone pin.

At **3014**, the clamp is locked to the bone fixation component. For example, the clamp may include a pair of jaws defining an aperture through which the bone fixation component may pass, and a locking device may be used to force the jaws to compress the bone fixation component in order to lock the clamp to the bone fixation component.

At **3016**, it is determined whether the bone fixation system is disposed in a desired orientation (e.g., position and/or angle relative to target joint, target bones, etc.). If the bone fixation system is not disposed in a desired orientation (e.g.,

the orientation is not acceptable), then at **3018**, clamp(s) may be unlocked, providing degrees of freedom allowing for adjustment of the bone fixation system and components of the bone fixation system.

In some embodiments, determining whether the bone fixation system is disposed in a desired orientation includes comparing an observed joint status of the target joint to a desired joint status of the target joint. For example, a clinical goal for the joint may include a particular joint status (e.g., a degree of flexure of the joint, relative angles of the bones about the joint, etc.) to be achieved using the bone fixation system.

If it is determined that the bone fixation is disposed in a desired orientation, then at **3020**, it is determined whether an additional bone pin needs to be attached. If it is determined that an additional bone pin is needed, then the procedure outlined in steps **3010**, **3012**, **3014**, **3016**, and **3018** may be followed to provide an additional clamp and attach an additional bone pin.

If it is determined that an additional bone pin is not needed, then at **3022**, angle(s) between various components in the bone fixation system, such as between a first fixation component and a second fixation component, may be adjusted.

At **3024**, after adjusting angles of the bone fixation system, it is determined whether the bone fixation system is disposed in a desired orientation. If it is determined that the bone fixation system is not disposed in a desired orientation, then at **3026**, any locked clamp(s) and bone fixation component(s) are unlocked, allowing for adjustment of the orientation of the bone fixation system, such as by adjusting angle(s) between bone fixation components. An angle of a clamp relative to a bone fixation component may be adjusted, such as by adjusting an angle defined by a longitudinal axis of the bone fixation component and a plane transverse to a through-bore of the clamp in which the bone fixation component is received. A position of the clamp relative to the bone fixation component may be adjusted as well, such as by shifting and/or sliding the bone fixation component and the clamp relative to one another.

In some embodiments, the bone fixation system is configured to be fixated about a target ankle joint. The bone fixation system includes a first frame which may be aligned about a first target bone of the lower extremity adjacent to the target ankle joint. The bone fixation system also includes a second frame which may be aligned to at least partially surround the target ankle. For example, the second frame may include an inferior frame portion and a posterior frame portion. Fixating such a bone fixation system may include aligning the first frame with a first target bone of the lower extremity, aligning the second frame such that the inferior frame is disposed in an inferior position relative to the target ankle joint and such that the posterior frame is disposed in a posterior position relative to the target ankle joint, aligning a first clamp with the first target bone, attaching a first bone pin to the first target bone using the first clamp as a drill guide, and locking the first clamp to the first frame. In some embodiments, such a bone fixation system may be further fixated by aligning a second clamp with a second target bone (e.g., a bone of the foot or of the heel), attaching a second bone pin to the second target bone using the second clamp as a drill guide, and locking the second clamp to the second frame.

If it is determined that the bone fixation system is disposed in a desired orientation, then at **3028**, all clamp(s) and bone fixation component(s) are locked. For example, locking devices may be used to lock clamp(s) to respective bone

fixation component(s). In some embodiments, bone fixation components may be engaged and locked using fasteners or other engagement devices as disclosed herein.

B. Clamping Devices and Systems with Locking Assembly  
Referring now to FIGS. **71-76B**, various embodiments of a clamping device **3100** including a locking assembly are shown. The clamping device **3100** can be similar to the clamp systems **300**, **400**, **500**, and/or **2600** described herein, with the exception of the features described further below, including the lever mechanism and jaw structures.

In some embodiments, a clamping device (or system) includes a clamp body and a locking assembly. The clamp body includes a first jaw and a second jaw, and defines a first channel configured to accommodate a fixation element (e.g., an external fixation rail, external fixation components described herein such as external fixation component **102**, etc.) along a longitudinal axis of the first channel. The first jaw defines a first opening and the second jaw defines a second opening. The locking assembly includes a first locking element, a second locking element, and a lever configured to couple to the second locking element. The first locking element includes a first end and a shaft portion extending from the first end. The shaft portion is sized to pass through the first opening and the second opening. The second opening is sized to restrict the first end from passing through the second opening. The first locking element defines a second channel sized to receive a bone pin. The locking assembly is configured to reduce a distance between the first jaw and the second jaw responsive to rotation of the second locking element relative to the first locking element. The lever is configured to be attached to the second locking element and rotated about the second locking element from a first position to a second position to cause the distance between the first jaw and the second jaw to be reduced further while the first end is in contact with the second opening.

Referring now to FIG. **71**, a clamping device **3100** includes a clamp body **3102** and a locking assembly **3108**. The clamp body **3102** includes a first jaw **3104** and a second jaw **3106**. The locking assembly **3108** includes a lever **3110** (e.g., an extension, a rotatable actuator). The locking assembly is configured to receive a bone pin **600**. The clamp body **3102** can define a first channel configured to accommodate a fixation element along a longitudinal axis of the first channel. The first channel can be defined between surfaces of the first jaw **3104** and the second jaw **3106** (e.g., surfaces that face each other). The longitudinal axis can pass through the first channel, and can be equidistant from some, most, or all points of the surfaces of the first jaw **3104** and second jaw **3106** that define the first channel.

Referring now to FIGS. **72A-72B**, the bone pin **600** can be received through the lever **3110** into a remainder of the locking assembly **3100** and the clamp body **3102**. Features of the locking assembly **3100** configured to receive, couple to, secure, clamp, and/or manipulate the bone pin **600** are described further herein. As shown in FIGS. **72A-72B**, the lever **3110** defines a lever channel **3111**. The lever channel **3111** can receive the bone pin **600**. The lever channel **3111** can be sized to accommodate the bone pin **600** (e.g., the lever channel **3111** has a diameter or a maximum dimension defined across the lever channel **3111** that is greater than a diameter or maximum dimension defined across the bone pin **600**. The lever channel **3111** can have a lever channel radius that is greater than or equal to a radius of an inner surface of a shaft portion of a first locking element of the locking assembly **3100** (see, e.g., first locking element **3120** of FIG. **73A**). The lever channel **3111** can help a user guide



## 31

the bone pin 600 through the locking assembly 3100 to a point on a patient to which the bone pin 600 is to be attached. For example, the bone pin 600 may be placed or rested against the lever 3110 to stabilize the bone pin 600 and align the bone pin 600 with the lever channel 3111 (and the channel 3134 of the locking assembly 3100). The lever channel 3111 can be coaxial with the channel 3134 to receive the bone pin 600 from the channel 3134. While FIGS. 72A-72B illustrate the bone pin 600 as being inserted first through a first end of the clamping device proximal to the first jaw 3104, in some embodiments, the bone pin 600 may also be inserted through a second end of the clamping device proximal to the second jaw 3106.

Referring now to FIGS. 73A-73D, various components of embodiments of the clamping device 3100 are illustrated. The locking assembly 3108 can include a first locking element 3120, a second locking element 3140, and a third locking element 3160. The components of the locking assembly 3108 can be configured to couple to one another, to receive the bone pin 600, and/or to apply forces to the clamp body 3102 causing the first jaw 3104 and second jaw 3106 to move closer to one another.

The first locking element 3120 can be similar to the shafts 306, 406, 2606 described herein. The first locking element 3120 is configured to surround a portion of the bone pin 600, and may include a flexible material allowing the first locking element 3120 to be compressed against the bone pin 600. The first locking element 3120 includes a first end 3122 and a shaft portion 3128 extending from the first end 3122. In some embodiments, the first end 3122 includes protrusions 3124 extending outward from the first end 3122. The protrusions 3124 can be received by a portion of the second jaw 3106, helping to align the first locking element 3120 with the second jaw 3106 and/or restrict motion of the first locking element 3120 relative to the second jaw 3106.

As shown in FIG. 73A, the first end 3122 has a spheroid shape (e.g., a shape defined such that most or all points on an exterior surface of the spheroid correspond to an ellipse rotated about one of its principle axes). In various embodiments, the first end 3122 can have various shapes (e.g., rectangular solid, cylindrical, shapes defined by a step function, conical or triangular solid). As described further herein with reference to FIG. 75A, the first end 3120 can define a maximum diameter that is greater than a minimum diameter of a second opening of the second jaw 3106, which can restrict motion of the first end 3122 relative to the second opening. The maximum diameter can be less than a shaft diameter of the shaft 3128.

The shaft portion 3128 is sized to pass through the first jaw 3104 and the second jaw 3106 (e.g., via openings of the first jaw 3104 and the second jaw 3106). The shaft portion 3128 can include an engagement feature configured to couple the first locking element 3120 to another component (e.g., the second locking element 3140). For example, FIG. 73A shows the engagement features as threads 3130; the engagement feature could additionally be or include recesses, protrusions, interdigitation, or other features configured to engage another component such that the first locking element 3120 may move together with the other component while engaged. The threads 3130 can extend along an outer surface of the first locking element 3120 adjacent to a second end 3126 of the first locking element 3120 opposite the first end 3122.

In some embodiments, the first locking element 3120 defines a channel 3134 sized to accommodate the bone pin 600. For example, a maximum dimension across the channel 3134 can be greater than a maximum dimension across the

## 32

bone pin 600. The first locking element 3120 and/or the channel 3134 can define a longitudinal axis 3136 (e.g., a channel axis) passing through the channel 3134. The longitudinal axis 3136 can be equidistant from some or all of the points of the channel 3134 (e.g., from an inner surface or wall of the first locking element 3120 defining the channel).

In some embodiments, the first locking element 3120 includes extensions 3132 (e.g., slits, protrusions). The extensions 3132 extend inward from the first end 3122 and the shaft portion 3128 (e.g., from an inner surface or wall of the first locking element 3120 defining the channel 3134). The extensions 3132 can be configured to apply a force against the bone pin 600 in response to compression of the first locking element 3120 (e.g., as the first locking element 3120 is tightened or compressed by the second locking element 3140 or the second jaw 3106).

Referring further to FIG. 73B, the second locking element 3140 can include a second locking element body 3142. The second locking element body 3142 can be sized to receive the shaft portion 3128 of the first locking element 3120. The second locking element body 3142 is shown to have a cylindrical shape to facilitate rotation of the second locking element body 3142 in a compact space; however, in various embodiments, the second locking element body 3142 can have other shapes (e.g., polygonal, rectangular).

The second locking element 3140 includes at least one rotational coupler element 3144 extending from the second locking element body 3142. The rotational coupler elements 3144 are configured to couple to (e.g., engage) the lever 3110, such that the lever 3110 can be rotated about the second locking element body 3142. For example, the second locking element 3140 and/or the rotational coupler elements 3144 can define a rotational axis 3150 passing through the second locking element 3140 about which the lever 3110 can rotate.

The second locking element 3140 includes an inner surface 3146 defining a channel in which the shaft portion 3128 of the first locking element 3120 can be received. For example, a maximum dimension across the channel (e.g., from a first point on the inner surface 3146 to a second point opposite the first point) can be greater than or equal to a maximum dimension of an outer surface of the shaft portion 3128. The inner surface 3146 includes an engagement feature configured to couple to or engage with the first locking element 3120. The engagement feature may be complementary to an engagement feature of the first locking element 3120. For example, as shown in FIG. 73B, the inner surface 3146 includes thread receiving members 3148 configured to engage the threads 3130 of the first locking element 3120. The second locking element 3140 and/or the inner surface 3146 can define a longitudinal axis 3152. The longitudinal axis 3152 may be equidistant from some, most, or all points on the inner surface 3146. The longitudinal axis 3152 may be in the same plane as and/or perpendicular to the rotation axis 3150. In some embodiments, the lever 3110, when coupled to the rotational coupler elements 3144, can apply a force to the rotational coupler elements 3144 in a direction perpendicular to the longitudinal axis 3152, causing the second locking element 3120 to rotate about the longitudinal axis 3152. In some embodiments, the locking assembly 3108 defines an engagement axis along which the bone pin 600 is received. The second locking element 3140 may be rotated about the engagement axis. For example, the engagement axis may coincide with the longitudinal axes 3136, 3152 when the second locking element 3140 is engaged to the first locking element 3120.

As the thread receiving members **3148** engage the threads **3130** of the first locking element **3120**, the second locking element **3140** can be coupled, engaged, attached, and/or secured to the first locking element **3120**. The longitudinal axis **3152** may align with the longitudinal axis **3136** when the first locking element **3120** is received in the channel of the second locking element **3140** (e.g., when the thread receiving members **3148** engage the threads **3130**).

The engagement of the receiving members **3148** and the threads **3130** may restrict motion between the first locking element **3120** and the second locking element **3140**. For example, when the thread receiving members **3148** engage the threads **3130**, a force applied to the first locking element **3120** along the longitudinal axis **3136**, or to the second locking element **3140** along the longitudinal axis **3152**, may be insufficient (e.g., less than a threshold force that is significantly greater than can be applied to the locking elements **3120**, **3140** by a typical user) to cause the first locking element **3120** to move along the longitudinal axis **3152** relative to the first locking element **3120**. Instead, rotation of the second locking element **3140** about the shaft portion **3128** of the first locking element **3120**, due to the engagement of the threads **3130** and the thread receiving members **3148**, allows the first locking element **3120** to be translated through the second locking element **3140**. In some embodiments, a portion of the shaft portion **3128** having the threads **3130** includes a material that is flexible or compressible, such that engaging the second locking element **3140** to the first locking element **3120** about the threads **3130** (or another engagement feature) flexes, bends, or compresses the shaft portion **3128** against the bone pin **600** (e.g., the extension **3132** may be forced against the bone pin **600**), which can increase locking of the bone pin **600**.

Referring now to FIG. 73C, the third locking element **3160** can include a base portion **3162**. The base portion **3162** is attachable to the first jaw **3104** (e.g., to a surface of the first jaw **3104** opposite the second jaw **3106**). The third locking element **3160** can include a receiving portion **3164** extending from the base portion **3162**. The receiving portion **3164** defines a cavity **3166**. The cavity **3166** is configured or sized to receive the second locking element **3140**. For example, a maximum dimension across the cavity **3166** can be greater than a maximum dimension across the second locking element **3140**.

The receiving portion **3164** can include or define a receiving wall **3168**. As described further with reference to FIGS. 74A-74B, the receiving wall **3168** can be shaped or sized to receive or match a cam wall of the lever **3110** (e.g., a curvature of the receiving wall **3168** is complementary to a corresponding curvature of the cam wall). As the lever **3110** is rotated about the second locking element **3140**, the lever **3110** applies a varying force against the receiving wall **3168**, which can cause the third locking element **3160** to move relative to the second locking element **3140** and/or apply a force against the first jaw **3104**. In some embodiments, features of the third locking element **3160** may be excluded, or may be incorporated in the lever **3110** or the second locking element **3140**. For example, the lever **3110** may be configured to attach to the first jaw **3104**, such that rotation of the lever **3110** against the first jaw **3104** causes a varying force to be applied to the first jaw **3104**.

As shown in FIG. 73D, the lever **3110** includes a cam wall **3112**. An inner surface **3202** of the cam wall **3112** (e.g., a surface facing towards the lever channel **3111**) and/or an inner cam wall **3204** defines a center **3206**. The inner surface **3202** and the inner cam wall **3204** are shaped, configured, and/or sized to engage the rotational coupler elements **3144**

of the second locking element body **3142**. For example, a radius of curvature of the inner cam wall **3204** and/or the inner surface **3202** can match (e.g., is equal to or is greater than an amount less than a threshold amount, resulting in a fit between the lever **3110** and the rotational coupler element **3144**) a radius of curvature of the rotational coupler elements **3144**. As the lever **3110** rotates about second locking element **3140**, the rotation axis **3140** of the second locking element **3140** aligns with the center(s) **3206** of the lever **3110**.

In some embodiments, the lever **3110** includes a tab wall **3210**. The tab wall **3210** is configured to be received by a corresponding tab receiver **3212** of the third locking element **3160**. For example, when the lever **3110** is rotated about the rotation axis **3150** of the second locking element **3140** to the second position, the tab receiver **3212** can be coupled to or secure the tab wall **3210**, restricting rotation of the lever **3110** towards the first position. In addition, the tab wall **3210** can provide a user with a lever arm to facilitate rotation of the lever **3110** both about the longitudinal axis **3152** of the second locking element **3140** when the second locking element **3140** is being threaded onto the first locking element **3120** to translate the first locking element **3120** through the second locking element **3140** (e.g., translate the first locking element **3120** in a direction from the clamp body **3102** towards the second locking element **3140**), and about the rotation axis **3150** as the lever **3110** is rotated from the first position towards the second position. In some embodiments, a length of the lever **3110** (e.g., from the center **3206** to a point at which the tab wall **3210** terminates) is greater than a threshold length required to apply sufficient force to rotate the lever **3110** from the first position to the second position to clamp the fixation element and the bone pin **600**, and less than a length (e.g., a greatest length) of the third locking element **3160** and/or a length (e.g., a greatest length) of the clamp body **3102**, providing a compact, effective mechanism for clamping the fixation element and the bone pin **600** (e.g., securing positions and/or orientations of the fixation element and the bone pin **600** relative to one another in space).

Referring now to FIGS. 74A-74B, various features of the engagement and interaction between the lever **3110**, the third locking element **3160**, and the clamp body **3102** are illustrated. The cam wall **3112** defines a first radius  $r_1$ , and a second radius  $r_2$ . The second radius  $r_2$  is greater than the first radius  $r_1$ . The radii  $r_1$ ,  $r_2$  can be defined from a center of rotation of the cam wall **3112**. The center of rotation of the cam wall **3112** may correspond to a center of an inner surface of the cam wall **3112** (see FIG. 73D) (e.g., a center that is equidistant from some, most, or all points on an inner cam wall configured to couple to the rotational coupler element **3144**, such that when the lever **3110** rotates about the second locking element **3140**, the rotation axis **3150** of the second locking element **3140** coincides with the center of the inner surface and/or the center of rotation).

In some embodiments, the lever **3110** is configured to rotate from a first position or orientation (e.g., a position or orientation as shown in FIG. 74A, in which the lever channel **3111** is aligned with a longitudinal axis of the bone pin **600**) to a second position. The second position may be a position or orientation as shown in FIG. 74B, in which the cam wall **3112** may be flush with the receiving wall **3168** and/or the lever **3110** can be secured by a retaining feature of the third locking element **3160**. The second position or orientation may be any other position or orientation as the lever **3110** is rotated between the position shown in FIG. 74A and the position shown in FIG. 74B. The rotation from the first

position to the second position may occur about the center of rotation of the cam wall 3112, such as when the lever 3110 is coupled to the second locking element 3140, such that the lever 3110 rotates about the rotation axis 3150 of the second locking element 3140. As the lever 3110 rotates from the first position to the second position, the radius of the cam wall 3112 in contact with a contact point 3170 of the receiving wall 3168 increases from the first radius  $r_1$  to the second radius  $r_2$ .

In embodiments, configurations, and/or arrangements of the clamping device 3100 in which the third locking element 3160 is attached to the first jaw 3104, the first end 3122 of the first locking element 3120 is in contact with the second jaw 3106 on a side of the second jaw 3106 opposite the first jaw 3104, the second locking element 3140 is engaged to the first locking element 3120, and the lever 3110 is coupled to the second locking element 3140, the distance between the center of rotation of the lever 3110 and the first end 3122 is fixed such that the increase in radius of the cam wall 3112 contacting the receiving wall 3168 increases a distance between the second locking element 3140 and the base portion 3162, causing the first end 3122 to pull the second jaw 3106 towards the first jaw 3104 to offset the increased distance between the second locking element 3140 and the base portion 3162. In some embodiments, the increased distance between the second locking element 3140 and the base portion 3162 is equal to a radius difference  $\Delta r$  between the first radius  $r_1$  and the second radius  $r_2$  the offset distance by which the second jaw 3106 moves towards the first jaw 3104 may be equal to the radius difference  $\Delta r$ .

In some embodiments, the clamping device 3100 can include a lock release member 3169. The lock release member 3169 is configured to releasably engage, lock, secure, attach, or otherwise couple the lever 3110 to the third locking element 3160. For example, the lock release member 3169 can be configured to apply a force to a first side of the lever 3110 opposite where the lever 3110 is received by the third locking element 3160 to hold or secure the lever 3110 in position. In some embodiments, the lock release member 3169 is or includes actuation member, such as a button, configured to engage or disengage the lever 3110 responsive to actuation (e.g., responsive to being pushed or pulled). In some embodiments, the lock release member 3169 is or includes a key configured to be slidably received and removed from a slot of the third locking element 3160. In some embodiments, the lock release member 3169 can facilitate selective locking of the clamping device 3100, such as to allow a medical professional performing a procedure using the clamping device 3100 to lock or unlock the lever 3110 to make adjustments to the clamping device 3100; the lock release member 3169 may be configured such that only the medical professional may actuate the lock release member 3169, such as when the lock release member 3169 is a key.

Referring now to FIGS. 75A-75B, various features of interactions between the components of the clamping device 3100 are illustrated. The first jaw 3104 defines a first opening 3107 (e.g., an interior wall or inner wall defines the first opening 3107). The first opening 3107 is sized to receive the shaft portion 3128 of the first locking element 3120. For example, the shaft portion 3128 can define a shaft dimension 3129 (e.g., a radius as illustrated, or a corresponding diameter) in a direction perpendicular to the longitudinal axis of the shaft portion 3128 (e.g., longitudinal axis 3136 shown in FIG. 73A). The first opening 3107 can define a first diameter 3188 (e.g., a first wall diameter) that is greater than or equal to the shaft diameter 3129, and a

second diameter 3190 (e.g., a second wall diameter) that is greater than the first diameter 3188. In some embodiments, such as shown in FIGS. 75A-75B, a profile of the first opening 3107 is smooth (e.g., macroscopically smooth, while in other embodiments, the first opening 3107 may have a profile defined by a step function or non-smooth or non-continuous profile). For example, the first opening 3107 may be defined by a conical inner surface of the first jaw 3104.

Gaps or spaces between the wall defining the first opening 3107 and the shaft portion 3128 may define a range of motion, such as for tilting the first locking element 3120 (and thus the bone pin 600 when the first locking element 3120 has received the bone pin 600). The range of motion may be based on an angle  $\alpha$  defined between a first portion of the wall having the first diameter 3188, and a second portion of the wall having the second diameter 3190 or another diameter greater than the first diameter 3188. In some embodiments, the angle  $\alpha$  is approximately 165 degrees (e.g., 150 degrees; greater than 90 degrees and less than or equal to 180 degrees; greater than or equal to 120 degrees and less than or equal to 175 degrees; greater than or equal to 135 degrees and less than or equal to 170 degrees; greater than or equal to 140 degrees and less than or equal to 160 degrees). In some embodiments, such as shown in FIG. 75A, the second portion of the wall having the second diameter 3190 may be angled relative to the first portion of the wall having the first diameter 3188 to define a tilt angle  $\beta$ . The tilt angle  $\beta$  may represent a range of motion by which the first locking element 3120 may be tilted relative to an orientation in which a longitudinal axis 601 of the bone pin 600, or the corresponding longitudinal axes of the first locking element 3120 and/or the second locking element 3140, are perpendicular to a plane 3192 that is parallel to surfaces of the first jaw 3104 and the second jaw 3106, and/or a plane that is parallel to outer rims of the first opening 3107 or the second opening 3109. For example, if the angle  $\alpha$  is 165, then the tilt angle  $\beta$  may be 15 degrees, such that the first locking element 3120 may tilt by 15 degrees (e.g., the first locking element 3120 may tilt by a 30 degree range of conical motion) when the outer surface of the shaft portion 3128 of the first locking element 3120 is in contact with the wall defining the first opening 3107. As further described with reference to FIGS. 76A-76B, allowing the first locking element 3120 to tilt or otherwise be oriented throughout a range of motion (e.g., a conical range of motion) within the first opening 3107 may advantageously allow a user to dynamically arrange the clamping device 3100, and thus an external fixation system utilizing the clamping device 3100, in arrangements or configurations during assembly of the external fixation system that are not possible with existing solutions (which may require fixing an angle between a fixation element and a bone pin throughout the assembly process). In some embodiments, the first opening 3107 is conical.

The second jaw 3106 defines a second opening 3109. In some embodiments, while the shaft portion 3128 of the first locking element 3120 is sized or configured to pass through the second opening 3109, the second opening 3109 is sized or configured to restrict or prevent the first end 3122 of the first locking element 3120 to pass through the second opening 3109 (e.g., be moved from a first side of the second opening 3109 opposite the first jaw 3104 to a second side of the second opening 3109 adjacent to the first jaw 3104). In such embodiments, if a force is applied to the first locking element 3120 in a direction that would move the first end 3122 towards the first jaw 3104 while the first end 3122 is

in contact with the second opening **3109** (e.g., with a wall of the second jaw **3106** defining the second opening **3109**), the force will be transmitted from the first end **3122** to the second jaw **3106**. The first locking element **3120** may thus cause the second jaw **3106** to move towards the first jaw **3104**.

In some embodiments, the clamp body **3102** includes a first material that is flexible (e.g., bends or otherwise changes in shape in response to a mechanical force). In response to a force applied to the second jaw **3106** by the first end **3122**, the clamp body **3102** may be reduced in size (e.g., the second jaw **3106** may move towards the first jaw **3104**; a distance between the second jaw **3106** and the first **3104** may decrease). As the second jaw **3106** moves towards the first jaw **3104**, a clamping force applied to a fixation element received in the first channel between the jaws **3104**, **3106** may be increased, increasing security of the fixation element. In some embodiments, the first end **3122** includes a second material that is flexible. The first material of the clamp body **3102** may be more flexible than the second material of the first end **3122**, such that any bending, flexing, or other change in shape that occurs in response to a force applied by the first end **3122** to the second jaw **3106** will predominantly (or totally) result in movement of the second jaw **3106** towards the first jaw **3104**. The first material of the clamp body **3102** may be located between the first jaw **3104** and the second jaw **3106**, acting as a pivoting member for movement of the second jaw **3106** towards the first jaw **3104**.

In some embodiments, the first end **3122** may include a second material that is flexible or compressible. The second material may be more flexible or compressible than a wall defining the second opening **3109**. As a force is applied by the first end **3122** against the second opening **3109**, some or all of the force may cause the first end **3122** to compress or flex away from the second opening **3109** (e.g., compress or flex inwards), thus transmitting the force to the bone pin **600** and increasing a clamping force for securing the bone pin **600**. In some embodiments, where the first locking element **3120** includes slits **3132**, the force applied by the first end **3122** against the second opening **3109** may additionally or alternatively cause the slits **3132** to move towards the bone pin **600**, similarly increasing a clamping force for securing the bone pin **600**. The second material may be configured to be compressed in a plane orthogonal to the channel **3134** in response to a force applied by the second opening **3109** against the first end **3122**.

The second opening **3109** (e.g., a wall defining the second opening **3109**) can include a first portion defining a first diameter **3180** (e.g., a dimension across the second opening **3109**) that is greater than a maximum diameter **3184** (e.g., a dimension across the first end **3122**, a dimension perpendicular to longitudinal axis **3136** of the first locking element **3120**) of the first end **3122**, and a second portion defining a second diameter **3182** that is less than a minimum diameter **3186** (e.g., a dimension across the first end **3122**, a dimension perpendicular to a longitudinal axis **3136** of the first locking element **3120**) of the first end **3122**. As such, the first end **3122** may not pass any further through the second opening **3109** towards the first jaw **3104** once the minimum diameter **3186** of the first end **3122** contacts the second diameter **3182**. The second diameter **3182** can be closer to the first jaw **3104** than the first diameter **3180**, such that the second portion is configured to restrict the first end **3122** from being moved further towards the first jaw when the first end is in contact with the second portion.

As further described with regards to FIGS. **76A-76B**, the first end **3122** may be tilted within the second opening **3109**, allowing the bone pin **600** to be tilted (e.g., to be tilted throughout a conical path or conical range of motion). In some embodiments, the range of tilting may be determined based on at least one of the first diameter **3180** of the second opening **3109**, the second diameter **3182** of the second opening **3109**, the first diameter **3188** of the first opening **3107**, and/or the second diameter **3190** of the first opening **3109**. In other words, the space defined by the first opening **3107** and/or the space defined by the second opening **3109**, enable the first locking element **3120** to be re-oriented within the first opening **3107** and the second opening **3109**.

Referring further to FIGS. **75A-75B**, and back to FIGS. **74A-74B**, as the lever **3110** rotates from the first position to the second position, the portion of the cam wall **3112** contacting the receiving wall **3168** of the third locking element **3160** increases in radius from  $r_1$  to  $r_2$ , increasing the distance between the center of rotation of the lever **3110** and the base portion **3162**. As the second locking element **3140** is fixed to the lever **3110** (e.g., when the lever **3110** is rotatably coupled to the second locking element **3140**), increasing the distance between the center of rotation of the lever **3110** and the base portion **3162** increases a distance **3114** between the second locking element **3140** and the third locking element **3160** (and/or between the second locking element **3140** and the clamp body **3102**), such as to move the second locking element **3140** away from the clamp body **3102**. While the second locking element **3140** is engaged to the first locking element **3120** (e.g., while thread receiving members **3148** engage threads **3130** of the first locking element **3120**), the distance between the second locking element **3140** and the first end **3122** may be fixed, resulting in a force causing the first end **3122** to move towards the first jaw **3104**, where force is transmitted to the second jaw **3106**. The distance **3114** may be equal to the radius difference  $\Delta r$  as the lever **3110** rotates from the first position to the second position.

Referring further to FIGS. **75A-75B**, in some embodiments, the clamp body **3102** includes at least one engagement member **3117** extending from an outer surface of the first jaw **3104** (e.g., a surface of the first jaw **3104**). For example, the clamp body **3102** can include an annular protrusion **3116** similar to the annular protrusion **312** or the annular protrusion **512** described herein that terminates in engagement members **3117**. The base portion **3162** of the third locking element **3160** may include at least one engagement receiving feature **3161** configured to engage the engagement members **3117**. In some embodiments, the engagement receiving feature **3161** is configured to ratchet, such that the third locking element **3120** may be rotated in a first direction (e.g., clockwise), but not in second direction (e.g., counter-clockwise). In some embodiments, the engagement members **3117** include at least one of interdigitation or radial serrations. In some embodiments, the third locking element **3160** is configured to selectively engage first jaw **3104** (e.g., only when the lever **3110** is in the second position), allowing the bone pin **600** to be tilted unless then third locking element **3160** is engaged to the first jaw.

Referring now to FIGS. **76A-76B**, the range of motion defined by the first opening **3107** and/or the second opening **3109** (see FIGS. **75A-75B**) allow the first locking element **3120**, and thus the bone pin **600**, to be rotated (e.g., conically rotated, tilted, conically tilted), enabling a user to arrange the clamping device **3100** in a variety of orientations while assembling the clamping device **3100**. When the lever **3110** is brought to the second position, the additional security

39

and/or locking provided may also secure the clamping device 3100 in an orientation where the bone pin 600 is tilted. For example, the clamping device 3100 may be assembled while the lever 3110 is in the first position, at which point the first locking element 3120 may still be tilted; when the lever 3110 is brought to the second position, then additional security and/or locking may apply a sufficient force to restrict further tilting of the first locking element 3120.

Clamping devices and systems manufactured in accordance with the embodiments disclosed herein can improve external fixation by providing a compact, elegant mechanism to clamp, lock, or otherwise secure a bone pin and an external fixation element (e.g., a rail) relative to one another. For example, such systems can allow a surgeon or other user to arrange the components of the clamping system in a desired orientation, rotate the second locking element about the first locking element to tighten the components of the system, perform any additional adjustments or movements that may be necessary, and then complete the locking of the system by rotating the lever from the first position to the second position, which can take advantage of the lever arm provided by the lever to increase the force that can be applied to compress and tighten against the bone pin and rail, while maintaining a form factor that is compact and/or has a low profile, reducing the opportunity for contact with surrounding components or the environment to disturb the clamping of the bone pin and rail.

The principles, preferred embodiments and modes of operation of the present invention have been made apparent in the foregoing description.

Although the embodiments are numbered with, for example, "first," "second," or "third," or "fourth," the ordinal numbers do not imply priorities of the embodiments.

Since many modifications, variations and changes in detail can be made to the described embodiments of the invention, it is intended that all matters in the foregoing description and shown in the accompanying drawings be interpreted as illustrative and not in a limiting sense. Thus, the scope of the invention should be determined by the appended claims and their legal equivalents.

What is claimed is:

1. A locking assembly, comprising:

- a first locking component including a base, the base including a first surface and a cam receiver extending from the first surface to a cam receiver edge, the cam receiver configured to receive a cam, the cam receiver edge having a first edge point closest to the first surface, the first surface defining an opening which is not parallel to a plane passing through the cam receiver;
- a second locking component including a first end, a second end, and a shaft portion extending from the first end to the second end, the second locking component configured to be coupled to the first locking component to translate through the opening along a first axis;
- the cam including a cam edge and defining a center of rotation, a first radius extending from the center of rotation to a first point of the cam edge, and a second radius extending from the center of rotation to a second point of the cam edge, the second radius perpendicular to and less than the first radius, the cam defines a channel configured to receive a bone pin;
- the cam configured to be rotated along the cam receiver edge about a second axis which is not parallel to the first axis from a first position at which the center of rotation is spaced from the first edge point by the first

40

radius to a second position at which the center of rotation is spaced from the first edge point by the second radius.

2. The locking assembly of claim 1, wherein the second locking component includes one or more threads configured to engage corresponding thread receiving members of the first locking component to be rotated while being translated along the first axis.

3. The locking assembly of claim 1, wherein the cam receiver edge is concave.

4. The locking assembly of claim 1, wherein the cam includes a tab extending from the cam edge and the first locking component includes a tab receiver extending from the base, the tab receiver configured to removably secure the tab to the base when the cam is at the second position.

5. The locking assembly of claim 4, further comprising a lock release member configured to cause the tab receiver to release the tab.

6. The locking assembly of claim 1, wherein the channel is configured to contact the bone pin when the cam is at the first position.

7. The locking assembly of claim 1, wherein rotating the cam from the first position to the second position adjusts a distance between the first end of the second locking component and the center of rotation of the cam.

8. The locking assembly of claim 1, wherein the first axis is perpendicular to the second axis.

9. The locking assembly of claim 1, wherein the cam includes a second cam edge spaced from and parallel to the cam edge.

10. A surgical kit for an external fixator system, comprising:

- a first locking component including a base, the base including a first surface and a cam receiver extending from the first surface to a cam receiver edge, the cam receiver configured to receive a cam, the cam receiver edge having a first edge point closest to the first surface, the first surface defining an opening which is not parallel to a plane passing through the cam receiver;
- a second locking component including a first end, a second end, and a shaft portion extending from the first end to the second end, the shaft portion including at least one rotational engagement feature configured to be coupled to the first locking component to translate the second locking component through the opening along a first axis while being rotated about the first axis;
- the cam including a cam edge and defining a center of rotation, a first radius extending from the center of rotation to a first point of the cam edge, and a second radius extending from the center of rotation to a second point of the cam edge, the second radius perpendicular to and less than the first radius, the cam defines a channel configured to receive a bone pin;
- the cam configured to be rotated along the cam receiver edge about a second axis which is not parallel to the first axis from a first position at which the center of rotation is spaced from the first edge point by the first radius to a second position at which the center of rotation is spaced from the first edge point by the second radius.
- 11. The surgical kit of claim 10, wherein the first locking component includes one or more thread receiving members configured to engage the at least one rotational engagement feature of the second locking component.
- 12. The surgical kit of claim 10, wherein the cam receiver edge is concave.

13. The surgical kit of claim 10, wherein the cam includes a tab extending from the cam edge and the first locking component includes a tab receiver extending from the base, the tab receiver configured to removably secure the tab to the base when the cam is at the second position. 5

14. The surgical kit of claim 13, further comprising a lock release member configured to cause the tab receiver to release the tab.

15. The surgical kit of claim 10, wherein the channel is configured to contact the bone pin when the cam is at the first position. 10

16. The surgical kit of claim 10, wherein rotating the cam from the first position to the second position adjusts a distance between the first end of the second locking component and the center of rotation of the cam. 15

17. The surgical kit of claim 10, wherein the first axis is perpendicular to the second axis.

18. The surgical kit of claim 10, wherein the cam includes a second cam edge spaced from and parallel to the cam edge. 20

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